

Mathematical Biology (App Topic D)

Andrew Martin

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1 Introduction - Basic Ideas

1.1 Dimensional Analysis

Units on both sides of an equation have to be the same - they have to be dimensionally consistent.

For example Coulomb's Law - for the force between two particles with charges q_1 and q_2 respectively

$$F = k_e \frac{q_1 q_2}{r^2}$$

Where q_1, q_2 have units Q (Coulombs). r will have units $[L]$ - square braces will mean units
And $F \implies \frac{[M][L]}{[T]^2}$ So

$$\frac{[M][L]}{[T]^2} = \frac{[k_e][Q]^2}{[L]^2}$$
$$[k_e] = \frac{[M][L]^3}{[T]^2[Q]^2}$$

As an aside - we will denote temperature as $[\Theta]$

This means we can write any physical relationship as a dimensionless equation in form

$$f(\beta) = 0$$

Where β_i are dimensionless groups. E.g. if we have time, length, gravity and mass, we can form the dimensionless group

$$\frac{gT^2}{L}$$

since the units of them will cancel out (g has units L/T^2).

The mass can't be involved in this relationship since it can't form a dimensionless group. It is possible that we have 'forgotten' some other term which could contain mass also.

Meaning

$$f\left(\frac{gT^2}{L}\right) = 0$$

I.e. gT^2/L is a zero of the function, and hence

$$\frac{gT^2}{L} = k$$

Or we could rewrite as

$$T = \sqrt{\frac{kL}{G}}$$

Consider the power of an atomic bomb. We want to know the energy, we know that the function will have to relate to E (units $[ML/T^2]$), R (units $[L]$), t (units $[T]$), and the air density ρ (units $[M/L^3]$).

$$\begin{aligned}[E] &= \frac{[M][L]^2}{[T]^2} \\ \frac{[E]}{[\rho]} &= \frac{[L]^5}{[T]^2} \\ \frac{[E][t^2]}{[\rho]} &= [L]^5 \\ \frac{[E][t^2]}{[\rho][R^5]} &= [1]\end{aligned}$$

Where $[1]$ is dimensionless

And hence

$$\frac{[E][t^2]}{[\rho][R^5]} = k$$

We have graphs of the R at various T

$$\begin{aligned}R^5 &= \frac{E}{k\rho}t^2 \\ \implies R^5 &\propto t^2\end{aligned}$$

Since we know E is constant, k constant and ρ won't really change early on.

So if we take the logs

$$\begin{aligned}5 \log R &= 2 \log t + \text{const} \\ \log t &= \frac{5}{2} \log R + \text{const}\end{aligned}$$

Of course this doesn't tell us what k is, and this is the only problem.

1.2 Non-dimensionalisation and Scaling

We will mostly skip this part because we've done it a fair bit in past

An example for reynolds number - to obtain euler and stokes equations Navier-stokes

$$\begin{aligned}\nabla \cdot u &= 0 \\ \rho \frac{Du}{Dt} &= -\nabla p + \mu \nabla^2 u\end{aligned}$$

Where

$$\frac{Du}{Dt} = \frac{\partial u}{\partial t} + (u \cdot \nabla)u$$

Have a general length scale $x = L\hat{x}$, a velocity scale $u = U\hat{u}$ and a time scale $t = \frac{L}{U}\hat{t}$ (which we would inevitably get anyway), lastly the pressure scale $p = \pi\hat{p}$ (not the number - a parameter)

So we get

$$\begin{aligned}\nabla \cdot u &= 0 \\ \frac{U}{L} \nabla \cdot \hat{u} &= 0 \\ \hat{u} &= 0\end{aligned}$$

And the momentum equation LHS:

$$\rho \frac{Du}{Dt} = \rho \left(U \frac{\partial \hat{u}}{\partial \hat{t}} + \frac{U^2}{L} (\hat{u} \cdot \nabla) \hat{u} \right)$$

$$\rho \frac{U^2}{L} \left(\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} \right)$$

The RHS

$$-\nabla p + \mu \nabla^2 u$$

$$-\frac{\pi}{L} \nabla^2 \hat{p} + \frac{\mu U}{L^2} \nabla \hat{u}$$

Equating:

$$\rho \frac{U^2}{L} \left(\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} \right) = -\frac{\pi}{L} \nabla^2 \hat{p} + \frac{\mu U}{L^2} \nabla \hat{u}$$

$$\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} = -\frac{\pi}{\rho U^2} \nabla^2 \hat{p} + \frac{\mu}{\rho L U} \nabla \hat{u}$$

Note that

$$\frac{\mu}{\rho U L} = \frac{1}{Re}$$

And for large (infinite) Reynolds number

$$\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} = -\frac{\pi}{\rho U^2} \nabla^2 \hat{p}$$

$$\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} = -\nabla^2 \hat{p}$$

by letting $\pi = \rho U^2$

For the stokes equation we instead take small Reynolds number

$$\rho \frac{L^2 U^2}{\mu U L} \left(\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} \right) = -\frac{\pi L^2}{L \mu U} \nabla^2 \hat{p} + \nabla \hat{u}$$

$$\rho \frac{L U}{\mu} \left(\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} \right) = -\frac{\pi L}{\mu U} \nabla^2 \hat{p} + \nabla \hat{u}$$

$$Re \left(\frac{\partial \hat{u}}{\partial \hat{t}} + (\hat{u} \cdot \nabla) \hat{u} \right) = -\frac{\pi L}{\mu U} \nabla^2 \hat{p} + \nabla \hat{u}$$

$$0 = -\frac{\pi L}{\mu U} \nabla^2 \hat{p} + \nabla \hat{u}$$

$$0 = -\nabla^2 \hat{p} + \nabla \hat{u}$$

By letting $\pi = \mu U / L$.

This shows that with non-dimensionalisation, assumptions for the problem have to be taken into account. And you can get different equations (and more simple ones sometimes).

1.3 Types of Models

2 Biochemical Reactions

2.1 Mass Action

Consider a chemical reaction



Where k is the reaction constant. This is a one way reaction.

Standard notation is $[A] = a$ concentration of A , and likewise for $[B] = b$ and $[C] = c$.

Units:

- Moles per litre a.k.a Molar M (so thats a number per litre). SI would be moles per m^3 but Molar is more common. Sometimes there is mass per litre/metre cubed

The rate of change of product (in this case just production) over time will depend on: number of collisions of A, B multiplied by the probability of it being a successful collision (enough kinetic energy to initiate reaction).

Assume the probability, k , is constant, and the number of collisions is proportional to a, b . This gives

$$\frac{dc}{dt} = kab$$

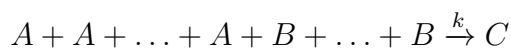
Which is the Law of Mass Action (we use Law loosely here - its just a model).

A reaction like this is called an 'Elementary reaction'

If you instead had a model of form



You can think of it like

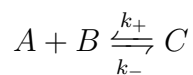


Then it would have equation:

$$\frac{dc}{dt} = ka^n b^m$$

(Addition \rightarrow power)

We also consider reversible reactions



Where k_+ is the forward reaction constant, and k_- is the backward reaction constant

$$\frac{dc}{dt} = k_+ab - k_-c$$

$$\frac{da}{dt} = -k_+ab + k_-c$$

$$\frac{db}{dt} = -k_+ab + k_-c$$

$$\frac{d(c+a)}{dt} = a$$

$$\frac{d(c+b)}{dt} = a$$

Since nothing is lost from the system (conservation of mass).

Hence

$$c(t) + a(t) = c_i + a_i$$

Where c_i, a_i are the initial quantities of c, a respectively.

And the same for b

$$c(t) + b(t) = c_i + b_i$$

And hence

$$a(t) = c_i + a_i - c(t)$$

$$b(t) = c_i + a_i - c(t)$$

Which we can plug into the $\frac{dc}{dt}$ DE.

2.2 Enzymes

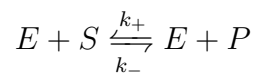
Proteins (mostly) which help speed up biochemical reactions (a biochemical catalyst) Particularly with the induced-fit theory (i.e. they fit the substrate/s, and then change shape to bind/separate substrate/s to give the product/s)

A particular enzyme is specific to a reaction (the lock-and-key).

They require very specific temperatures and pH levels to work - otherwise they will become denatured and won't be able to carry out the reaction (or will be less effective).

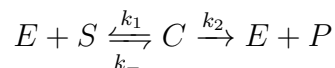
2.3 Michaelis-Menten Kinetics

Consider the enzymatic reaction



In this case E will be an enzyme, and is a catalyst since it isn't lost from the reaction, S is the substrate, and P is the product.

We know there is an intermediate step where the enzyme and substrate are 'reacted' together to form an intermediate complex, C , which then decays into E and P to finish the reaction:



This is the Michaelis-Menten scheme

We want to set up a system of ODEs for this scheme

$$\begin{aligned}\frac{ds}{dt} &= -k_1 es + k_- c \\ \frac{de}{dt} &= -k_1 es + k_- c + k_2 c \\ \frac{dc}{dt} &= k_1 es - k_- c - k_2 c \\ \frac{dp}{dt} &= k_2 c\end{aligned}$$

Note that the units of $k_1 = [1/Ct]$ (per time & concentration) are different from $k_- = [1/t]$ and $k_2 = [1/t]$.

Initial conditions

$$\begin{aligned} s(0) &= s_i > 0 \\ e(0) &= e_i > 0 \\ c(0) &= 0 \\ p(0) &= 0 \end{aligned}$$

So we also get

$$\frac{d(e+c)}{dt} = 0$$

So $e+c = e_i + c_i = e_i$ since $c_i = 0$ by our previous assumption.

So we can simplify the system quite quickly since we can ignore the e equation.

The reduced system

$$\begin{aligned} \frac{ds}{dt} &= -k_1 s(e_i - c) + k_- c = -k_1 s e_i + (k_1 s + k_-) c \\ \frac{dc}{dt} &= k_1 s(e_i - c) - k_- c - k_2 c = k_1 s e_i - (k_1 s + k_- + k_2) c \end{aligned}$$

With $s(0) = s_i$ and $c(0) = 0$. Which are two non-linear ODEs for s and c .

Allegedly $e_i \ll s_i$ usually, and so we can have a small parameter $\epsilon = \frac{e_i}{s_i}$ (Asymptotics coming back to haunt me)

Non-dimensionalise:

$$t = T\tilde{t}, \quad s = s_i\tilde{s}, \quad c = \epsilon s_i\tilde{c}$$

(And drop the tildes immediately)

$$\begin{aligned} \frac{s_i}{T} \frac{ds}{dt} &= -k_1 s_i s(\epsilon s_i - \epsilon s_i c) + (k_1 s_i s + k_-) \epsilon s_i c \\ &= -k_1 T s(\epsilon s_i - \epsilon s_i c) + (k_1 s_i s + k_-) \epsilon T c \\ \frac{ds}{dt} &= \epsilon k_1 s_i T (cs - s) + \epsilon k_- T c \end{aligned}$$

We want to choose the time scale relative to the time it takes to form product. I.e. we want $\frac{ds}{dt} = \mathcal{O}(1)$ So choose $T = \frac{1}{\epsilon k_1 s_i}$, and calling $\frac{k_-}{k_1 s_i} =: A$

$$\frac{ds}{dt} = cs - s + Ac$$

And plugging into the c DE

$$\epsilon \frac{dc}{dt} = s - cs - (A + B)c$$

Where $B := \frac{k_2}{k_1 s_i}$, and we will call $A + B = k_m = \frac{k_- + k_2}{k_1 s_i}$

$$\epsilon \frac{dc}{dt} = s - cs - k_m c$$

Take a perturbation series

$$\begin{aligned} s &= s_0 + \epsilon s_1 + \dots \\ c &= c_0 + \epsilon c_1 + \dots \end{aligned}$$

At $\mathcal{O}(1)$

$$\begin{aligned}
 \frac{ds_0}{dt} &= c_0 s_0 - s_0 + A c_0 \\
 0 &= s_0 - c_0 s_0 - k_m c_0 \\
 \implies c_0 &= \frac{s_0}{k_m + s_0} \\
 \implies \frac{ds_0}{dt} &= \frac{s_0^2}{k_m + s_0} - s_0 + \frac{A s_0}{k_m + s_0} \\
 &= \frac{1}{k_m + s_0} [s_0^2 - s_0(k_m + s_0) + A s_0] \\
 &= \frac{s_0}{k_m + s_0} [A - k_m] \\
 &= \frac{-B s_0}{k_m + s_0}
 \end{aligned}$$

B is often called V_{max} i.e. the max velocity of the reaction. And k_m is the concentration at which the uptake is $V_{max}/2$.

This solution is a Michaelis-Menten function.

We can solve this DE also (but its not very convenient):

$$\begin{aligned}
 \frac{ds_0}{dt} &= \frac{-B s_0}{k_m + s_0} \\
 \int \frac{k_m + s_0}{s_0} ds_0 &= Bt + \text{const} \\
 k_m \log(s_0) + s_0 &= -Bt + \text{const}
 \end{aligned}$$

Using the IC gives $1 = \text{const}$. So

$$k_m \log s_0 + s_0 = 1 - Bt$$

We have a problem that $c_0 \neq 0$. So we can't satisfy the IC. Since we killed the $\frac{dc}{dt}$ term.

This is known as a singular perturbation problem, since it is killing the highest derivative and changes the way the function operates. Whereas a regular perturbation problem is one where we don't get rid of the highest derivative.

So we can now consider this as a boundary layer problem like in Asymptotics. c will have some rapid growth at the start with the slower process after. So we would apply the same methods as before. I.e. we have an outer solution now but we need an inner solution.

To obtain the inner solution we have to rescale to reintroduce the highest derivative to leading order.

In this case we will only need to rescale time

$$T = \frac{t}{\epsilon}$$

Giving

$$\frac{d}{dt} = \frac{\partial T}{\partial t} \frac{\partial}{\partial T} = \frac{1}{\epsilon} \frac{\partial}{\partial T}$$

And hence

$$\begin{aligned}
 \frac{1}{\epsilon} \frac{\partial s}{\partial T} &= cs - s + Ac \\
 \frac{dc}{dT} &= s - cs - k_m c
 \end{aligned}$$

Same perturbation series idea

$$s = s_0 + \epsilon s_1 + \dots$$

$$c = c_0 + \epsilon c_1 + \dots$$

Giving

$$\frac{\partial s_0}{\partial T} = 0 \implies s_0 = \text{const} = 1$$

And for the c equation

$$\begin{aligned} \frac{dc_0}{dT} &= 1 - c_0 - k_m c_0 \\ &= 1 - (1 + k_m) c_0 \end{aligned}$$

Giving

$$c_{0,inner} = \frac{1 - e^{-(k_m+1)T}}{k_m + 1}$$

Get the composite solution (and overlap) - the composite for s_0 is what we had before

$$s_0 + k_m \log s_0 = 1 - Bt$$

For c_0

$$\begin{aligned} \lim_{T \rightarrow \infty} c_{0,inner} &= \lim_{t \rightarrow 0} c_{0,outer} \\ \lim_{T \rightarrow \infty} \frac{1 - e^{-(k_m+1)T}}{k_m + 1} &= \frac{1}{k_m + 1} = \frac{1}{1 + k_m} \end{aligned}$$

So the c_{comp} solution is

$$c_{comp} = \frac{1 - e^{-(k_m+1)t/\epsilon}}{k_m + 1} + \frac{s_0}{k_m + s_0} - \frac{1}{k_m + 1} = \frac{-e^{-(k_m+1)t/\epsilon}}{k_m + 1} + \frac{s_0}{k_m + s_0}$$

The concept of V - the reaction velocity is just

$$V = \frac{dp}{dt}$$

i.e. the rate of forming the final product (we would consider the dimensionless version but biochemists would write the dimensional version).

From the text (pg 9-16 of Mathematical Physiology) - we can see that enzymatic reactions can get quite complicated with varying effects and relationships between enzymes and substrates. It shows the effects of inhibition (competitive vs allosteric) and cooperativity

Terms:

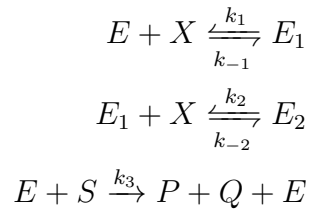
- Competitive inhibition - another compound can fit in the slot for the enzyme, inhibiting the reaction we are watching
- Allosteric inhibition - other active sites on the can be used by other compounds, changing the shape of the active site. This can prevent (or slow down) the reaction for the substrate we care about.

- A ligand is anything that binds to the enzyme and can either be called an effector or a modifier
- Cooperativity is when the enzyme can bind multiple sets of the substrate and run the reaction simultaneously. This gives rise to the hill equation

$$h(c) := \frac{c^n}{k + c^n}$$

Where n is (usually) an integer related to the number of substrates that can bind to the enzyme.

Example: For the reaction



The system of DEs (we care about s, x, e, e_1, e_2, p) would be

$$\begin{aligned} \frac{ds}{dt} &= -k_3 s e_1 \\ \frac{de}{dt} &= -k_1 e x + k_{-1} e_1 + k_3 e_1 s \\ \frac{dx}{dt} &= \alpha - \beta x - k_1 e x + k_{-1} e_1 x - k_2 e_1 x + k_{-2} e_2 \\ \frac{de_1}{dt} &= k_1 e x - k_{-1} e_1 - k_2 e_1 x + k_{-2} e_2 - k_3 e_1 s \\ \frac{de_2}{dt} &= k_2 e_1 x - k_{-2} e_2 \\ \frac{dp}{dt} &= k_3 e_1 s \end{aligned}$$

So the reaction velocity will end up as

$$V = k_3 e_1 s$$

Whatever that may be.

If we use a quasi-steady-state analysis. Assume we have a small amount of enzyme and a lot of substrate.

In this case that would mean the rate of production of e_1, e_2 is very small. I.e.

$$\begin{aligned} \frac{de_1}{dt} &\approx 0 \\ \frac{de_2}{dt} &\approx 0 \end{aligned}$$

Conservation (adding the e, e_1, e_2 equations and adding the s, p equations) gives

$$\begin{aligned} \frac{d}{dt}(e + e_1 + e_2) &= 0 \\ \frac{d}{dt}(s + p) &= 0 \end{aligned}$$

But the $s + p$ one is not entirely necessary.

Using the quasi-steady state analysis derive an equation for $\frac{dx}{dt}$. So let's write e and e_2 in terms of e_1

$$k_2 e_1 x = k_{-2} e_2 \implies e_2 = \frac{k_2 x e_1}{k_{-2}}$$

And in the e_1 equation

$$\begin{aligned} 0 &= k_1 e x - k_{-1} e_1 - k_2 e_1 x + k_{-2} e_2 - k_3 e_1 s \\ 0 &= k_1 e x + k_{-1} e_1 - k_3 e_1 s \\ e_1 &= \frac{k_1 x e}{k_{-1} + k_3 s} \end{aligned}$$

Plug into the e_2 statement, and plug into the x equation

$$e_2 = \frac{k_1 k_2 x^2 e}{k_{-2}(k_{-1} + k_3 s)}$$

$$\begin{aligned} \frac{dx}{dt} &= \alpha - \beta x - k_1 e x + k_{-1} e_1 - k_2 e_1 x + k_{-2} e_2 \\ \frac{dx}{dt} &= \alpha - \beta x - k_3 e_1 s \end{aligned}$$

Now use $e + e_1 + e_2 = \mu$ since they must be constant (mass action)

$$\begin{aligned} e + e_1 + e_2 &= \mu \\ e \left[1 + \frac{k_1 x}{k_{-1} + k_3 s} + \frac{k_1 k_2 x^2}{k_{-2}(k_{-1} + k_3 s)} \right] &= \mu \\ \frac{e}{k_{-1} + k_3 s} \left[k_{-1} + k_3 s + k_1 x + \frac{k_1 k_2 x^2}{k_{-2}} \right] &= \mu \end{aligned}$$

And going back to

$$\begin{aligned} \frac{dx}{dt} &= \alpha - \beta x - k_3 e_1 s \\ &= \alpha - \beta x - k_3 \frac{k_1 x e}{(k_{-1} + k_3 s)} s \\ &= \alpha - \beta x - k_3 k_1 x s \left[\frac{\mu}{k_{-1} + k_3 s + k_1 x + \frac{k_1 k_2}{k_{-2}} x^2} \right] \end{aligned}$$

Which is the form required by the question (after you do some non-dimensionalisation).

3 Excitable systems

Considering transport through the membrane of cells (active and passive).

Note that

- Excitable systems involve ions and molecules with some kind of charge with SI Coulomb (C).

- Total charge is always conserved
- Charges exert forces on one another (like charges repel, unlike attract). Electric potential V is the potential energy of a unit of charge due to such forces, measured in volts (V) or Joules per Coulomb (JC^{-1}).
- A concentration of positive particles has a large positive potential and a concentration of negative particles has a large negative potential
- Electrical current, I is defined as the rate of flow of charge measured in Amperes A (or equivalently Cs^{-1}).

3.1 Circuits

For a simple electric circuit

- $q(t)$ is the charge
- $I(t) = \frac{dq}{dt}$ is the current
- $V(t)$ is the potential difference (analogous to pressure in fluids)
- R is the resistance in Ohms Ω
- $g = \frac{1}{R}$ is the conductance
- C is the capacitance measured in Farads, F .

Mathematical Traits:

- Ohm's Law - the potential difference (a.k.a voltage drop) across a resistor is proportional to the current through the resistor

$$V_R(t) = IR = I \frac{1}{g}$$

- Faraday's Law - the potential difference across a capacitor is proportional to the charge stored

$$V_c(t) = \frac{q(t)}{C}$$

- Kirchoff's Law - the voltage supplied is equal to the total voltage drop

$$V(t) = V_R(t) + V_C(t) = \frac{I}{g} + \frac{q}{C}$$

(Looking at the circuit in the notes) For elements in parallel, the total current is the sum of the currents in the branches

$$\begin{aligned} I(t) &= I_1 + I_2 + I_3 \\ &= g_1V + g_2V + g_3V \end{aligned}$$

We have

$$\begin{aligned} V &= \frac{q}{C} \\ \frac{\partial V}{\partial t} &= \frac{1}{C} \frac{dq}{dt} \\ &= \frac{1}{C} I \\ &= \frac{V}{C} (g_1 + g_2 + g_3) \end{aligned}$$

3.2 Membrane Potential

We can't quite use $I = gV$ in a cell - instead we would use

$$I = g(V)(V - V^*)$$

So $g(V)$ is a function of V and V^* is a 'hurdle' - described below

Consider a system with a semi-permeable membrane dividing two regions - where both sides are neutrally charged with positive charges X^+ and negative charges Y^- . (one side could have more X and Y than the other) It allows X to pass through, but not Y . Say one side has more X and Y than the other. Some X will pass through the membrane via diffusion, to reduce the concentration gradient, but this movement generates a potential difference. There would be a point where the repulsion due to this potential would overcome the effects of diffusion. This potential is V^* (the Nernst potential) - the potential at which the diffusive flux is balanced by the electric-field generated flux. The Nernst potential will be a constant based on the ion as far as we're concerned.

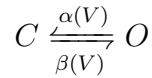
3.3 Gating

Exponentially it has been found that g is not constant, it depends on V and t .

As an example explanation - the channels to allow ion flow are not always open. The transition rate from closed to open will depend on V .

Now we write the membrane conductance as gn where n is the proportion of channels which are open.

The example of simple gating: Letting O denote open channels and C as closed channels, the reaction scheme is



Where $\alpha(V)$ and $\beta(V)$ represent the voltage dependent rates of opening/closing the gates. If we use the law of mass action

$$\frac{dn}{dt} = \alpha(V)(1 - n) - \beta(V)n$$

We can rewrite this as

$$\tau_n(V) \frac{dn}{dt} = n_\infty(V) - n$$

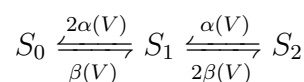
$$n_\infty(V) = \frac{\alpha}{\alpha + \beta}$$

$$\tau_n(V) = \frac{1}{\alpha + \beta}$$

Where n_∞ is the equilibrium value for n , and $\tau_n(V)$ is the timescale for approach to equilibrium (both of which can be obtained experimentally).

3.3.1 Multiple Gates

Assume now that each channel consists of multiple gates, each of which can be open or closed. Lets assume we have 2 gates of the same type, and S_i is the proportion of channels with i gates open. Then the reaction scheme is



Where the factors of 2 arise since there are two possible states with one gate open and one closed. Note that we have the overall constraint that

$$S_0 + S_1 + S_2 = 1$$

Using mass action kinetics to eliminate S_1 we get

$$\begin{aligned}\frac{dS_0}{dt} &= \beta(V)(1 - S_0 - S_2) - 2\alpha(V)S_0 \\ \frac{dS_2}{dt} &= \alpha(V)(1 - S_0 - S_2) - 2\beta(V)S_2\end{aligned}$$

Where in general V could be a function of time and space. The proportion of open gates n is given by

$$n = \frac{1}{2}S_1 + S_2 = \frac{1}{2}(1 - S_0 + S_2)$$

$$\begin{aligned}\frac{dn}{dt} &= -\frac{1}{2}\frac{dS_0}{dt} + \frac{1}{2}\frac{dS_2}{dt} \\ &= \alpha(V)(1 - n) - \beta(V)n\end{aligned}$$

Which is the same form as what we had for the simple gating scenario.

The system will be satisfied by

$$S_0 = (1 - n)^2, \quad S_1 = 2n(1 - n), \quad S_2 = n^2$$

We can show this by plugging these forms into the mass action solutions.

We can also verify that the system decays to this via a perturbation

$$\begin{aligned}S_0 &= (1 - n)^2 + z_0 \\ S_2 &= n^2 + z_2\end{aligned}$$

And substituting these into the S_0, S_2 equations and using $\frac{dn}{dt}$ we get

$$\begin{aligned}\frac{dz_0}{dt} &= -2\alpha z_0 - \beta(z_0 + z_2) \\ \frac{dz_2}{dt} &= -\alpha(z_0 + z_2) - 2\beta z_2\end{aligned}$$

Or in matrix notation

$$\frac{d}{dt} \begin{pmatrix} z_0 \\ z_2 \end{pmatrix} = \begin{pmatrix} -(2\alpha + \beta) & -\beta \\ -\alpha & -(\alpha + 2\beta) \end{pmatrix} \begin{pmatrix} z_0 \\ z_2 \end{pmatrix}$$

This matrix will have eigenvalues

$$\lambda_1 = -(\alpha + \beta), \quad \lambda_2 = -2(\alpha + \beta)$$

And so these DEs will exponentially decay to zero, and so we will decay to the solutions given before.

We can generalise this to k identical gates, the fraction of open channels will be n^k , where the n DE is the same as here.

And so the conductance for a channel with k identical gates will be

$$gn^k$$

3.3.2 Non-identical Gates

So now if we allow for non-identical gates in the channel. For now we will assume a channel with two types of gates, m, h . We will assume 2 m gates and 1 h gate. Let S_{ij} denote the proportion of channels with i of the m -gates open and j of the h -gates open. So there are 6 possible configurations for the channel. If we let m denote the proportion of open m gates and h be the proportion of open h gates,

Then using the law of mass action, we can show

$$\begin{aligned} S_{00} &= (1 - m)^2(1 - h) \\ S_{10} &= 2m(1 - m)(1 - h) \\ S_{20} &= m^2(1 - h) \\ S_{01} &= (1 - m)^2h \\ S_{11} &= 2m(1 - m)h \\ S_{21} &= m^2h \end{aligned}$$

So that the proportion of open channels is m^2h where m and h satisfy

$$\begin{aligned} \frac{dm}{dt} &= \alpha(V)(1 - m) - \beta(V)m \\ \frac{dh}{dt} &= \gamma(V)(1 - h) - \delta(V)h \end{aligned}$$

Where γ, δ are the rates of switching between the closed and open states for the h gates.

And the conductance will be gm^2h

3.4 Hodgkin-Huxley model

A model to explain the mechanisms underlying the electrical signals in the axon of a giant squid.

3.4.1 Structure of a Neuron

Effectively a Neuron is a cell with a nucleus with a large extruding ‘cable’ which is the axon, which then connects to a transmitter section.

When a cell becomes partially depolarised, a series of events takes place:

1. Upstroke phase - Sodium channels open in response to depolarisation allowing positively charged sodium ions to enter the cells, decreasing the polarisation until the cell becomes positively charged
2. Excited phase - on a slower timescale, potassium channels open, allowing potassium ions to leave. Sodium ions continue to enter and the potential difference falls (back to negative).
3. Downstroke phase - the cell becomes negatively charged and so the sodium channels close (making it even more negatively charged!) and so the cell is ‘hyperpolarised’
4. Refractory and Recovery Phases - The sodium channels are now mostly inactive, and slowly become active again until the cell returns to its original state.
5. Propagation - these impulses propagate down the axon through repetition. This gives us a **travelling wave**

3.4.2 Hodgkin-Huxley model

Let

- q - charge density per unit length
- C - capacitance of the membrane per unit area
- a - radius of the axon
- I_i - the outward current (rate of movement of ions) per unit area of membrane
- V - membrane potential

Since it is cylindrical, surface area of a unit length is $2\pi a$. So

$$q = 2\pi a C V \implies \frac{dq}{dt} = 2\pi a C \frac{dV}{dt}$$

We have several currents due to: capacitance, potassium, sodium, and leakage

$$I_C + 2\pi a I_{Na} + 2\pi a I_K + 2\pi a I_L = 0$$

Which is $= 0$ since charge must be conserved - and hence total current must be 0.

$$\implies 2\pi a C \frac{dV}{dt} = -2\pi a (I_{Na} + I_K + I_L)$$

$$\implies C \frac{dV}{dt} = -(I_{Na} + I_K + I_L)$$

From earlier in the course we expect the ionic currents to have form

$$I = g(V)(V - V^*)$$

I.e.

$$I_{Na} = g_{Na}(V)(V - V_{Na})$$

$$I_K = g_K(V)(V - V_K)$$

$$I_L = g_L(V - V_L)$$

Note that we have assumed that g_L does not depend on V

Hence

$$C \frac{dV}{dt} = -(I_{Na} + I_K + I_L)$$

$$C \frac{dV}{dt} = -[g_{Na}(V)(V - V_{Na}) + g_K(V)(V - V_K) + g_L(V - V_L)]$$

Introduce (kinda like the gates in a channel)

- m - the sodium activation variable
- h - the sodium inactivation variable
- n - the potassium activation

We somehow obtain

$$\begin{aligned}\tau_m(V) \frac{dm}{dt} &= m_\infty(V) - m \\ \tau_h(V) \frac{dh}{dt} &= h_\infty(V) - h \\ \tau_n(V) \frac{dn}{dt} &= n_\infty(V) - n\end{aligned}$$

For constant V , $m \rightarrow m_\infty(V)$ exponentially with time constant τ_m , and likewise for the others.

(From experimentation) the potassium conductance depends on n^4 , i.e. it is likely a four-gate channel, and Sodium depends on m^3h . Hence the conductances have form:

$$\begin{aligned}g_{Na} &= \bar{g}_{Na} m^3 h \\ g_K &= \bar{g}_K n^4\end{aligned}$$

We wont properly discuss the τ and ∞ functions because they are grotty but we don't really care.

We can simplify the system in to a pair of coupled equations.

$$C \frac{dV}{dt} = - (\bar{g}_{Na} m^3 h + \bar{g}_K n^4 + \bar{g}_L) (V - V_{eq})$$

Where

$$V_{eq} = \frac{\bar{g}_{Na} m^3 h V_{Na} + \bar{g}_K n^4 V_K + \bar{g}_L V_l}{\bar{g}_{Na} m^3 h + \bar{g}_K n^4 + \bar{g}_L}$$

Let $\nu = V - V_{eq}$

$$\begin{aligned}\frac{d\nu}{dt} &= -\frac{1}{C} (g_{Na}(\nu)(\nu - \nu_{Na}) + g_K(\nu)(\nu - \nu_K) + g_L(\nu - \nu_L)) \\ \tau_m(\nu) \frac{dm}{dt} &= m_\infty(\nu) - m \\ \tau_h(\nu) \frac{dh}{dt} &= h_\infty(\nu) - h \\ \tau_n(\nu) \frac{dn}{dt} &= n_\infty(\nu) - n\end{aligned}$$

We can obtain experimentation values for ν_K , ν_{Na} , ν_L , g_{Na} , g_K , g_L , C .

We can plot the τ 's and x_∞ 's. And we observer

$$\tau_m \ll \tau_h, \tau_n$$

So we can approximate by saying that $m \approx m_\infty(\nu)$.

Using numerics you find that

$$n + h \approx n_\infty + h_\infty \approx const = \bar{h} \approx 0.85$$

Use this to eliminate h.

We have reduced the system to 2 equations:

$$\begin{aligned}C \frac{d\nu}{dt} &= - [\bar{g}_{Na} m_\infty^3(\nu)(\bar{h} - n)(\nu - \nu_{Na}) + \bar{g}_K n^4(\nu - \nu_K) + \bar{g}_L(\nu - \nu_L)] \\ \tau_n(\nu) \frac{dn}{dt} &= n_\infty(\nu) - n\end{aligned}$$

We now take τ_n to be approximately constant, $\tau_n \approx \bar{\tau}_n = 5ms$. Also non-dimensionalise

$$\nu = \nu_{Na} \tilde{\nu}, \quad t = \bar{\tau}_n \tilde{t}$$

And immediately drop tildes.

$$\frac{dn}{dt} = n_\infty(\nu) - n = k(\nu, n)$$

$$\epsilon \frac{d\nu}{dt} = -g(\nu, n) = -[\gamma_K n^4(\nu + \nu_K^*) + \gamma_L(\nu - \nu_L^*) + m_\infty^3(\nu)(\bar{h} - n)(\nu - 1)]$$

The sign for ν_K^* changes because all of the non-dimensional parameters are positive even though the nernst potential for potassium is negative.

Where the new dimensionless parameters are $\epsilon, \gamma_K, \gamma_L, \nu_K^*, \nu_L^*$. And note that ϵ, γ_L are small parameters (except γ_L near ν_K^*)

To do proper analysis, we look for the fixed point(s). 2D system so look for intersection of nullclines. We get the fixed point at

$$\nu = 0, n = n_\infty(0) > 0$$

Take a linear perturbation near the fixed point

$$\nu = \hat{\nu}, n = n_\infty(0) + \hat{n}$$

Where $|\hat{\nu}|, |\hat{n}| \ll 1$. We get using taylor series

$$\frac{d}{dt} \begin{pmatrix} \hat{n} \\ \hat{\nu} \end{pmatrix} = \begin{pmatrix} k_n & k_\nu \\ -g_n/\epsilon & -g_\nu/\epsilon \end{pmatrix} \begin{pmatrix} \hat{n} \\ \hat{\nu} \end{pmatrix} = \mathbf{J} \begin{pmatrix} \hat{n} \\ \hat{\nu} \end{pmatrix}$$

And evaluate around $(n_\infty(0), 0)$.

Eigenvalues of the Jacobian

$$\text{tr} J = -1 - g_\nu/\epsilon, \quad \det J = \frac{g_\nu + n_\infty g_n}{\epsilon}$$

Noting that n_∞ was an increasing function so $n_{\infty_\nu} > 0$, and similarly g is increasing in ν .

$$\begin{aligned} g_n &= m_\infty^3(\nu)(1 - \nu) + 4n^3\gamma_K(\nu + \nu_K^*) \\ g_n(0, n_\infty(0)) &= m_\infty^3(0) + 4n_\infty^3(0)\gamma_K\nu_K^* > 0 \end{aligned}$$

We hence find

$$\text{tr} J < 0, \quad \det J > 0$$

Giving 2 eigenvalues with negative real parts - so this is a stable fixed point.

We drew some phase-plane diagrams here: Starting with the nullclines

$$\begin{aligned} \frac{\partial n}{\partial t} = 0 &\implies n = n_\infty(\nu) \\ \frac{d\nu}{dt} = 0 &\implies g(\nu, n) = 0 \\ g(\nu, n) = 0 &\implies \frac{n^4}{\bar{h} - n} = \frac{(1 - \nu)m_\infty^3(\nu)}{\gamma_K\nu_K^*(1 + \frac{\nu}{\nu_K^*})} \end{aligned}$$

Assuming γ_L is negligible(I think?)

We find that the ν nullcline has the same qualitative shape as the right-hand side since $\frac{n^4}{h-n}$ is monotonically increasing for $n < \bar{h}$. We get just the one fixed point ($\nu = 0, n = n_\infty(0)$). The ‘hump’ in the $g(\nu, n) = 0$ nullcline is where we can generate the large excursion from the fixed point. Noting that

$$\frac{\partial \nu}{\partial t} = -\frac{1}{\epsilon} g(\nu, n)$$

We get a large movement in the ν direction, until we hit the curve $g(\nu, n)$ and then we have increasing n and follow the hump to the top, and we cut through the $n = n_\infty(\nu)$ curve near horizontally, and then follow the $g(\nu, n)$ curve to the fixed point.

If we looked at ν against time in this trajectory, we would have a steep increase, a small decrease, a steep decrease into a negative value, and then a slow approach to $\nu = 0$. This significant change we call an ‘action potential’, since it would be related to the actual electrical pulse used by the body.

If we were to decrease ν to a point below the steady state.

3.5 Fitzhugh-Nagumo equations

They both wanted to essentially obtain a callnonical type form for action potential behaviour.

$$\epsilon \frac{d\nu}{dt} = A\nu(\nu - a)(1 - \nu) - w + I_{ext}^*, \quad \frac{dw}{dt} = -w + b\nu$$

w is kind of like if we had $w = n - n_{eq} = n - n_\infty(0)$ from before. Where I_{ext} is some external current

$$0 < A < \mathcal{O}(10)$$

$$0 < a < 1$$

b suff large.

Lets first consider the system with $I_{ext}^* = 0$

Nullclines:

$$w = A\nu(\nu - a)(1 - \nu)$$

$$w = b\nu$$

We want b suff large so that we only get 1 intersection here (as opposed to the possibility of 2 or 3.)

Plotting the nullclines (in the (ν, w) plane) makes the behaviour quite clear.

Taking $I_{ext} \neq 0$ will correspond to a vertical shift in the ν nullcline, making no real change to the behaviour (still excitable), unless I_{ext} is very large, where the excitable behaviour is lost. There is a ‘sweet spot’ for I_{ext} such that the w nullcline intersects in-between the humps of the ν nullcline, which gives an orbital which keeps looping (an oscillation). Changing the value of b will change the slope of the w nullcline, potentially giving 2, 3 intersections (fixed points) (as said before).

4 Partial differential equation models

Obviously we care about space and time so ODEs are too boring for this course.

4.1 Conservation Equations

If we have some closed volume V inside of the domain \mathcal{D} , with V 's surface S , with a 'chemical concentration' (doesn't have to be a concentration, but for the sake of argument. Density would also work) $c(\mathbf{x}, t)$. c will have to have units of 'amount of stuff' per unit volume

Then the total amount of stuff in V will be

$$\text{total stuff in } V = \iiint_V c dV$$

Stuff can only leave V through its surface, S . So any change in c will be due to

- Production/loss
- entering/leaving via S

Hence

$$\frac{\partial}{\partial t} \iiint_V c dV = - \iint_S \mathbf{J} \cdot \hat{\mathbf{n}} dS + \iiint_V f(\mathbf{x}, t) dV$$

Where

- \mathbf{J} is the flux of c (number of molecules crossing a unit area per unit time)
- $\hat{\mathbf{n}}$ is the unit outward normal to S
- $f(\mathbf{x}, t)$ is the rate of production/loss of c per unit volume

Note the minus sign in the flux term. This is since $\hat{\mathbf{n}}$ points outward

Using the divergence theorem:

$$\iint_S \mathbf{u} \cdot \hat{\mathbf{n}} dS = \iiint_V \nabla \cdot \mathbf{u} dV$$

We get

$$\frac{\partial}{\partial t} \iiint_V c dV = - \iiint_V \nabla \cdot \mathbf{J} dV + \iiint_V f(\mathbf{x}, t) dV$$

Since V was just some arbitrary volume, then this must be true at every point within \mathcal{D} , and hence for all point \mathbf{x} in \mathcal{D} :

$$\frac{\partial c}{\partial t} + \nabla \cdot \mathbf{J} = f(\mathbf{x}, t)$$

Which is the mass conservation equation. The tricky usage of this is using the right form of \mathbf{J} and f - using physical intuition and modelling skills

4.2 Physical processes of advection and diffusion

4.2.1 Diffusion

Where something naturally moves through a volume solely based on a concentration gradient. Random motion at a molecular level (Brownian motion). It tends to even out concentration gradients (differences). Diffusion is temperature dependent - faster at higher temperatures, since the amount of energy is increased, the number of interactions increases. The simplest assumption you could make for diffusion is that the flux is proportional to the concentration gradient, i.e.

$$\mathbf{J} = -D \nabla c$$

Where D is the diffusion coefficient (based on temperature but usually we hold temperature constant). This is called **Fick's Law**. 'Law' is used loosely once again - it is a simple model. It tends to be extremely accurate with most experimental observations however. A regular diffusion model would be (if we assumed $f = 0$, and $J = -D\nabla C$).

$$\frac{\partial c}{\partial t} = \nabla \cdot (D\nabla c)$$

If D is a constant then we get

$$\frac{\partial c}{\partial t} = D\nabla^2 c$$

4.2.2 Advection

Advection is the movement of something due to a flow, and hence it will occur in the direction of flow. If a chemical is only transported by advection through a fluid (and there is no diffusion)

$$\mathbf{J} = c\mathbf{v}$$

Where \mathbf{v} is the fluid velocity

In reality - chemicals can (and will) diffuse through flowing fluids - hence we look into advection-diffusion effects, i.e.

$$\mathbf{J} = c\mathbf{v} - D\nabla c$$

4.3 Reaction-advection-diffusion equations

We will consider advective-diffusive scenarios where chemical reactions are also occurring. So we get the equation

$$\frac{\partial c}{\partial t} + \nabla \cdot (c\mathbf{v}) = \nabla \cdot (D\nabla c) + f(c, \mathbf{x}, t)$$

Where

- $c(\mathbf{x}, t)$ is the dependent variable to solve (chemical concentration, cell density, etc.)
- \mathbf{v} is the fluid velocity vector (usually given)
- $D(\mathbf{x}, t)$ is the diffusion coefficient
- $f(c, \mathbf{x}, t)$ is the source/degradation/reaction term.

If we wanted to non-dimensionalise the RAD equation.

- L - characteristic length-scale of the problem (usually size of the domain, \mathcal{D})
- c_0 - characteristic concentration scale
- U - characteristic fluid velocity scale

So we get

$$\mathbf{x} = L\tilde{\mathbf{x}}, \quad c = c_0\tilde{c}, \quad \mathbf{v} = U\tilde{\mathbf{v}}$$

But for t, f , if we have a constant D :

$$t = \frac{L^2}{D}\tilde{t}, \quad f = \frac{Dc_0}{L^2}\tilde{f}$$

Then, dropping tildes, we get

$$\frac{c_0 D}{L^2} \frac{\partial c}{\partial t} + \frac{U c_0}{L} \nabla \cdot (c \mathbf{v}) = \frac{c_0 D}{L^2} \nabla^2 c + \frac{D c_0}{L^2} f$$

And hence:

$$\frac{\partial c}{\partial t} + \mathcal{P} \nabla \cdot (c \mathbf{v}) = \nabla^2 c + f$$

Where

$$\mathcal{P} = UL/D = \frac{T_{diff}}{T_{adv}} \implies \frac{\text{adv importance}}{\text{diff importance}}$$

Is the Péclet number, representing the relative importance of advection compared to diffusion.

If we assume incompressible flow also (which often holds true)

$$\nabla \cdot \mathbf{v} = 0$$

Then we get

$$\frac{\partial c}{\partial t} + \mathcal{P}(\mathbf{v} \cdot \nabla)c = \nabla^2 c + f$$

Many models assume only one spatial dimension (and this tends to be a good approximation).

4.4 Diffusion and Random Motion

We have to look at how the diffusion equation actually expresses random motion. As a formal formulation Considering a collection of particles moving randomly along a line in one dimension. If we divide time into discrete steps δt and in that time a particle moves δx either right with probability p_r or left with probability p_l . Assuming there is no bias ($p_r = p_l = \frac{1}{2}$). Let $c(x, t)\delta x$ be the number of particles in the segment $[x, x + \delta x]$ at t . Then

$$c(x, t + \delta t) = c(x, t) + p_r c(x - \delta x, t) - p_r c(x, t) + p_l c(x + \delta x, t) - p_l c(x, t)$$

By conservation. Taking taylor expansions in space and time give

$$\begin{aligned} c(x, t + \delta t) &= c(x, t) + \delta t \frac{\partial c}{\partial t} + \frac{1}{2}(\delta t)^2 \frac{\partial^2 c}{\partial t^2} + \dots \\ c(x \pm \delta x, t) &= c(x, t) \pm \delta x \frac{\partial c}{\partial x} + \frac{1}{2}(\delta x)^2 \frac{\partial^2 c}{\partial x^2} + \dots \end{aligned}$$

Substituting this into the conservation equation (and using $p_r = p_l = \frac{1}{2}$) gives

$$\delta t \frac{\partial c}{\partial t} + \mathcal{O}(\delta t^2) = \frac{1}{2}(\delta x)^2 \frac{\partial^2 c}{\partial x^2} + \mathcal{O}(\delta x)^4$$

Dividing through by δt and take limit as $\delta t \rightarrow 0$ and making (the rather bold) assumption:

$$\lim_{\delta t \rightarrow 0} \frac{(\delta x)^2}{2\delta t} = D$$

We get (to leading order)

$$\frac{\partial c}{\partial t} = D \frac{\partial^2 c}{\partial x^2}$$

We could also consider biased movement, but that's a little messy.

4.5 Reaction-Advection models

Assuming we can ignore diffusion, we have a simpler model.

4.5.1 Membrane Oxygenator

Consider cardiac surgery where it is necessary to bypass the heart to perform the procedure. Circulation must be maintained artificially, using a heart-long machine, which uses a membrane oxygenator which pumps blood through a membrane to allow oxygenation and carbon dioxide removal before returning blood to the body

An ideal membrane oxygenator is: a thin gas permeable membrane separates blood and gas flows in the circuit, oxygen diffuses from the gas side into the blood and carbon dioxide the other way around for disposal. An important issue is to understand how long it takes for the blood to be reoxygenated. If we consider this in $1D$ where the blood stream has diameter d , and velocity v_b and the gas has velocity v_g , both in the x direction. We assume:

- blood is incompressible
- gas flows much faster than blood ($v_g \gg v_b$) so that the concentration of oxygen (C_g) in the gas is approximately constant
- The concentration of oxygen in the blood is a function of position x and time t only.
- Advection is the dominant transport process (neglect diffusion)
- Transport of oxygen from gas to blood is proportional to the concentration difference.

By conservation of mass, the oxygen concentration in the blood $C(x, t)$ is given by

$$\frac{\partial C}{\partial t} + v_b \frac{\partial C}{\partial x} = h(C_g - C)$$

Where h is a transfer coefficient. Note that h has units of $[T]^{-1}$ and hence is a timescale for oxygen transfer. To complete the system we require an IC and BC. We will take

$$C(x, 0) = f(x), \quad C(0, t) = g(t)$$

And assume blood enters at $x = 0$ with constant oxygen concentration $C_0 < C_g$. Similarly at $t = 0$ we assume all the blood is at C_0 .

To solve this we non-dimensionalise based on timescale T , so that we get

$$t = T\tilde{t}, \quad x = \frac{v_b}{h}\tilde{x}, \quad C = C_g\tilde{C}$$

And the dimensionless equation is then

$$\tau \frac{\partial C}{\partial \tilde{t}} + \frac{\partial C}{\partial \tilde{x}} = 1 - C$$

Where $\tau = 1/hT$ is the ratio of the timescale of oxygen transfer to the timescale of interest. The B/I Cs become $C(0, t) = C(x, 0) = C_i$ where $C_i = C_0/C_g < 1$.

We assume $\tau \ll 1$ since we assume this will happen after a short start-up time. and find a solution C which is just a function of x . We get

$$\frac{\partial C}{\partial x} = 1 - C, \quad C(0) = C_i$$

With solution

$$C = 1 + (C_i - 1)e^{-x}$$

And as $x \rightarrow \infty$, $C \rightarrow 1$, i.e. the oxygen concentration tends to that of the gas.

Lets say we need the concentration to reach some fraction, C^* , of the gas (we would be given this value). Then we solve

$$C^* = 1 + (C_i - 1)e^{-L}$$

And hence

$$L = \log \left| \frac{1 - C_i}{1 - C^*} \right|$$

And if we redimensionalise we get, for required dimensional length l

$$l = \frac{v_b}{h} \log \left| \frac{C_g - C_0}{C_g(1 - C^*)} \right|$$

Since we have made so many assumptions, we need to think about how accurate this answer really is. We have neglected diffusion, and assumed constant velocity. Are they physically sensible?

Real fluids will have varying velocity across the channel, maximised at the centre and zero at the walls (known as Poiseuille flow). Hence blood near the wall requires less distance to reoxygenate than that near the center which is moving faster. Hence this sets up a gradient, and implies diffusion could be significant. This is known as Taylor dispersion.

4.5.2 Age-structured model for Chemotherapy

Let $n(a, t)$ be the number of malignant cells with ages (or cell cycle stages) a at time t . Total number of cells at time t

$$\int_0^\infty n(a, t) da$$

After a small time δt , the age or maturity increases by $\delta a = \delta t$.

By conservation

$$n(a, t + \delta t) = n(a, t) + n(a - \delta a, t) - n(a, t) - \mu(a, t)n(a, t)\delta t$$

Where $\mu(a, t)$ is a death rate for cells.

Some rearranging:

$$\begin{aligned} n(a, t + \delta t) &= n(a, t) + n(a - \delta a, t) - n(a, t) - \mu(a, t)n(a, t)\delta t \\ \frac{n(a, t + \delta t) - n(a, t)}{\delta t} &= \frac{n(a - \delta a, t) - n(a, t)}{\delta t} - \mu(a, t)n(a, t) \\ \frac{n(a, t + \delta t) - n(a, t)}{\delta t} &= \frac{n(a - \delta a, t) - n(a, t)}{\delta a} \frac{\delta a}{\delta t} - \mu(a, t)n(a, t) \\ \frac{n(a, t + \delta t) - n(a, t)}{\delta t} &= \frac{n(a - \delta a, t) - n(a, t)}{\delta a} - \mu(a, t)n(a, t) \\ \lim_{\delta t \rightarrow 0} \frac{n(a, t + \delta t) - n(a, t)}{\delta t} &= \lim_{\delta a \rightarrow 0} \frac{n(a - \delta a, t) - n(a, t)}{\delta a} - \mu(a, t)n(a, t) \\ \frac{\partial n}{\partial t} &= -\frac{\partial n}{\partial a} - \mu(a, t)n \\ \frac{\partial n}{\partial t} + \frac{\partial n}{\partial a} &= -\mu(a, t)n \end{aligned}$$

Which is a reaction-advection equation known as Von Foerster's equation. Its like for the reaction term, instead of spatial variable x , we have a , and the velocity is the constant, 1.

To solve the PDE we need a BC and an IC

$$n(a, 0) = f(a), \quad n(0, t) = \int_0^\infty b(a)n(a, t)da$$

Where $f(a)$ is the initial age distribution, and $b(a)$ is the birth rate of cells for cells at age a . Of course we expect $b(a) = 0$ for $a < a_1$ and $a > a_2$.

For the this example, assume that when cell reaches maturity, $a = 1$, the cell divides to produce two new cells at age $a = 0$ (so the original cell dies). This means

$$n(0, t) = 2n(1, t)$$

I.e. we've picked $b(a) = 2\delta(a - 1)$ where $\delta(x)$ is the delta function, 0 everywhere except $x = 0$ where it is unity.

$$n(a, 0) = N_0\gamma(a)$$

Where N_0 is the initial number of cells, and $\gamma(a)$ is the age distribution s.t

$$\int_0^1 \gamma(a)da = 1$$

Now to finally consider the chemo part. We would want μ to target an age bracket to kill cells (a cell cycle specificity). In this case, we will instead consider $\mu(a, t) = \mu(t)$, i.e. the drug that kills cells based on time rather than age.

This allows us to look for separable solutions (as not all μ 's would)

$$n(a, t) = f(t)w(a)$$

Substitution into the PDE gives

$$\begin{aligned} f'w &= -fw' - \mu(t)fw \\ \frac{f'}{f} + \mu(t) &= -\frac{w'}{w} = \lambda \end{aligned}$$

Where λ is a constant.

And hence solutions for f

$$f' = (\lambda - \mu)f \implies f = Ae^{\lambda t}e^{-M(t)}$$

Where $M(t) = \int_0^t \mu(\tau)d\tau$ and A is an arbitrary constant. w gives

$$w' = -\lambda w \implies w = Be^{-\lambda a}$$

And After some tidying

$$n(a, t) = Ce^{\lambda t - M(t) - \lambda a}$$

Where C, λ are constants to be determined.

Use the BC/IC to get them

$$\begin{aligned}
 n(a, 0) &= N_0 \gamma(a) = C e^{-\lambda a} \\
 \int_0^1 N_0 \gamma(a) da &= \int_0^1 C e^{-\lambda a} da \\
 N_0 &= -\frac{C}{\lambda} e^{-\lambda a} \Big|_{a=0}^{a=1} \\
 &= -\frac{C}{\lambda} e^{-\lambda-1} \\
 C &= \frac{\lambda N_0}{1 - e^{-\lambda}}
 \end{aligned}$$

And the BC

$$\begin{aligned}
 n(0, t) &= 2n(1, t) \\
 C e^{\lambda t - M(t)} &= 2e^{-\lambda} C e^{\lambda t - M(t)} \\
 1 &= 2e^{-\lambda}
 \end{aligned}$$

And so $\lambda = \log 2$

And hence

$$n(a, t) = 2 \log 2 N_0 e^{\log 2(t-a) - M(t)}$$

If we take

$$N(t) = \int_0^1 n(a, t) da$$

Will then find

$$\frac{n(0, t)}{N(t)} = \text{const}$$

4.6 Reaction Diffusion Models

We see a lot more of these than reaction-advection models.

A simple model for embryo culture in vitro (Yvonne Stokes was working on this!)

We put cells in an open tube (to allow oxygen in) within a medium of some sort (some fluid/gas) which is not moving and hence any movement through the medium to the cells will be via diffusion

Consider only one dimension (x up the tube), and the oxygen concentration. The oxygen concentration in the tube is $c(x, t)$, we will have a constant partial pressure of oxygen outside of the tube P_a (partial pressure is based on the total pressure and the concentration of the thing [oxygen]). I.e. if the pressure was P and there was a concentration $Y\%$ of oxygen, then the partial pressure would be PY . Cells are well mixed through the tube.

Want to know how high the partial pressure P_a has to be to sustain the cells.

The flux J will be given by Fick's Law, i.e.

$$J(x, t) = -D(x, t) \frac{\partial C}{\partial x}$$

And we have a rate of oxygen consumption $Q(x, t)$ And hence we get

$$\frac{\partial C}{\partial t} = \frac{\partial}{\partial x} \left(D \frac{\partial C}{\partial x} \right) - Q$$

We assume D is a constant:

$$\frac{\partial C}{\partial t} = D \frac{\partial^2 C}{\partial x^2} - Q$$

We need an IC, $C(x, 0) = C_0 = \text{constant}$ and we need two boundary conditions. We will need no oxygen flux at $x = 0$ and continuity for the partial pressure at $x = h$ where h is the top of the medium, so we get

$$\frac{\partial C}{\partial t}(0, t) = 0, \quad \gamma C(h, t) = P_a$$

Henry's law relates concentration and partial pressure as we have used above: where $P = \gamma C$, P is the partial pressure, C is the concentration and γ is Henry's law constant which is medium dependent (partial pressure in air P_a is assumed to be constant)

Since we are looking over a long timespan (days, weeks, etc.) look for steady state solutions, i.e. solutions to

$$D \frac{\partial^2 C}{\partial x^2} - Q(x, t) = 0$$

Q constant is easy to solve, but not very good since it isn't very informative and you could get negative solutions. So we could try using $Q = kC$ for some constant k since it makes sense that the consumption relates to concentration. If C_0 is big a better choice is the Michaelis-Menten function.

$$Q = \frac{Q_{max}C}{K_m + C}$$

We won't solve this here now though

5 Travelling Waves

We motivate this with the wound healing assay.

We grow cells in a dish so that they cover the whole dish (confluent), and then we generate a wound by scraping a section of cells away. The cells then migrate and proliferate forming a moving front to 'invade' the wounded, unoccupied region to close the wound. Let the direction of movement (normal to the scrape) be x and look at cell density. You basically get a constant density to the left of the scrape and a zero density to the right, and then (against time) a travelling wave will form to fill in the gap in the plot.

The model is generated with Fisher's equation (reaction-diffusion)

$$\frac{\partial n}{\partial t} = D \nabla^2 n + \mu n \left(1 - \frac{n}{K}\right)$$

Where $n(\mathbf{x}, t)$ is the number of cells at \mathbf{x} , at time t . So $D \nabla^2 n$ is diffusion - random movement of cells. $\mu n(1 - \frac{n}{K})$ proliferation of cells (birth rate), where K is a carrying capacity and μ is the max proliferation rate (max birth rate).

Take \mathbf{x} as x (1D case) We want to non-dimensionalise, so take

$$t = \frac{\tilde{t}}{\mu}, \quad x = \sqrt{\frac{D}{\mu}} \tilde{x}, \quad n = K \tilde{n}$$

And, dropping tildes gives

$$\frac{\partial n}{\partial t} = \frac{\partial^2 n}{\partial x^2} + n(1 - n)$$

letting $x = 0$ be the boundary of the wound, the conditions are

$$x \rightarrow -\infty, \quad n(x, t) \rightarrow 1, \quad x \rightarrow \infty, \quad n(x, t) = 0$$

We know that it will grow in waves, i.e. the shape of the solution remains the same, but in time it will 'move' along. So we look for travelling wave solutions.

Take the travelling wave ansatz

$$n(x, t) = \phi(x - ct) = \phi(z)$$

Where c is the (constant) wave speed

The boundary conditions for ϕ

$$\phi(-\infty) = 1, \quad \phi(\infty) = 0$$

Sub ϕ into fishers equation

$$\begin{aligned} \frac{dn}{dt} &= \frac{\partial^2 n}{\partial x^2} + n(1 - n) \\ -c \frac{d\phi}{dz} &= \frac{d^2 \phi}{dz^2} + \phi(1 - \phi) \end{aligned}$$

Write as two first order ODEs

$$\begin{aligned} \phi' &= \psi \\ \psi' &= \phi^{(2)} = -c\psi - \phi(1 - \phi) = g(\phi, \psi) \end{aligned}$$

Look for fixed points:

$$\phi' = 0, \quad \psi' = 0 = f(\phi, \psi)$$

Clearly $\psi = 0$ is the ϕ nullcline, and $\phi = 0, \phi = 1$ are the intersecting psi nullclines Hence two fixed points

$$(\phi, \psi) = (0, 0), \quad (1, 0)$$

Stability: Get the Jacobian

$$J = \begin{pmatrix} f_\phi & f_\psi \\ g_\phi & g_\psi \end{pmatrix} = \begin{pmatrix} 0 & 1 \\ 2\phi - 1 & -c \end{pmatrix}$$

Eigenvalues satisfy

$$\begin{aligned} \det(J - \lambda I) &= 0 \\ \lambda^2 - \text{tr}(J)\lambda + \det J &= 0 \\ \lambda &= \frac{\text{tr}(J) \pm \sqrt{\text{tr}(J)^2 - 4 \det J}}{2} \end{aligned}$$

At $(0, 0)$

$$J = \begin{pmatrix} 0 & 1 \\ -1 & -c \end{pmatrix}$$

$\text{tr}(J) = -c$ and $\det(J) = 1$. Since trace is the sum and det the product of the eigenvalues, we have two with negative real parts. Which is a stable fixed point.

$$\lambda = \frac{c \pm \sqrt{c^2 - 4}}{2}$$

Note that $c^2 \geq 0$ for $c \geq 2$. We know $c \geq 0$ due to the boundary condition. So there is a bifurcation at $c = 2$. If we have $c < 2$ then we have complex eigenvalues, and hence this is a stable spiral. If $c > 2$ we have real eigenvalues, and we have a stable node.

At $(1, 0)$,

$$J = \begin{pmatrix} 0 & 1 \\ 1 & -c \end{pmatrix}$$

$\text{tr}(J) = -c$ and $\det(J) = -1$. Since $\det < 0$ we have one negative and one positive, and hence it is a saddle point.

$$\lambda = \frac{c \pm \sqrt{c^2 + 4}}{2}$$

Note that $\phi = 1$ is for $z = -\infty$ and $\phi = 0$ is for $z = \infty$, so we wanted trajectories that go from $\phi = 0$ to $\phi = 1$.

The saddle point will have a stable direction and an unstable direction.

For the $(0, 0)$ fixed point we have the two outcomes, stable node and stable spiral. For the stable node ($c \geq 2$), the trajectories will connect from the unstable direction of the saddle, straight to the node (along an arc). This is a realistic result.

For the stable spiral ($c < 2$), the trajectories are more interesting, since the signs of ϕ, ψ will change when ϕ gets close to 0. So plotting ϕ against z will have some oscillation towards $\phi \rightarrow 0$. This is a physically unrealistic result, since cell density must be > 0 .

So for physically relevant solutions, we must have $c \geq 2$.

I.e. there is a minimum wavespeed, c^* , which is exactly the value where $(0, 0)$ changes from spiral to a node; $c^* = 2$.

The travelling wave (TW) solution close to $(0, 0)$ can be described by the linearisation from the Jacobian.

$$\lambda_{1,2} = -\frac{c}{2} \pm \frac{c}{2} \sqrt{1 - \frac{4}{c^2}}$$

So for $c = c^* = 2$ we get

$$\lambda_1 = \lambda_2 = -1$$

With mult. 2

The eigenvector for the linearised problem around $(0, 0)$ with $c = c^*$

$$\begin{pmatrix} \phi \\ \psi \end{pmatrix} = e^{-z}(c_1 + c_2 z) \begin{pmatrix} 1 \\ -1 \end{pmatrix}$$

Near $(0, 0)$ the solution decays like e^{-z} , i.e. like e^{-x+ct} , which will behave like e^{-x} as $x \rightarrow \infty$. Note this is the non-dimensional x (without the tilde because we've been lazy) We had

$$x = \sqrt{\frac{D}{\mu}} \tilde{x}, \quad c = \sqrt{\frac{D}{\mu}} \mu \tilde{c} = \sqrt{D\mu} \tilde{c}$$

So redimensionalising:

$$e^{-\tilde{x}} = e^{-\sqrt{\frac{\mu}{D}} x}, \quad c^* = 2\sqrt{D\mu}$$

Where $\sqrt{\frac{\mu}{D}}$ is the decay rate of the solution for dimensional $x \rightarrow \infty$.

$$\sqrt{\frac{\mu}{D}} = \frac{c^*}{2D}$$

This is all assuming $c = c^*$ for this solution.

6 Keller-Segel Model

6.1 Motivation

Slime moulds - potentially a bridge between primitive unicellular life forms and multicellular organisms. One of the best studied is *Dictyostelium discoideum* which lives as hundreds of thousands of single amoeboid cells in the soil. When food runs low a series of events occurs:

1. They form aggregation sites - cells move toward focal points in pulsing, wave-like manners
2. These sites form multicellular 'blobs' known as slugs.
3. The slug moves as a single body despite all cells being independent
4. Cells near the front become **prestalk** cells, while those near the end become **prespores**.
5. The slug finds a suitable environment
6. It changes shape - it acts as a 'reverse fountain', the prestalk cells move around the outside and down through the centre of the cell mass giving a slender stalk, supporting a spore-filled capsule
7. The stalk cells harden and die, but allow the spore cells to be carried on air currents to favourable environments to propagate the species.
8. This is a form of self-sacrifice.

The starving slime mould cells secrete a chemical called cyclic AMP (cAMP) which is attractive to other cells. Free cAMP in the extra-cellular environment promotes cAMP secretion by other cells. The cells also secrete an enzyme *phosphodiesterase* which degrades cAMP.

6.2 Assumptions

- In the absence of chemical signals the *dictyostelium* cells move around at random
- Cells are attracted to cAMP, so they tend to move from places with low cAMP concentration to ones with high.
- During the aggregation process, proliferation & death are negligible.
- Each cell produces cAMP (we will assume at a constant rate)
- cAMP is degraded in the environment (assume at a rate proportional to its concentration)

Consider 1D with $0 \leq x \leq L$ Let $a(x, t)$ be the cell density and $c(x, t)$ be the cAMP concentration.

Since cells move at random, for a random movement coefficient (random motility) μ , and then move against the cAMP gradient (towards higher cAMP) we get:

$$\frac{\partial a}{\partial t} = \mu \frac{\partial^2 a}{\partial x^2} - \frac{d}{dx} J_{adv}$$

We have assumed the advection is proportional to the cAMP concentration, in multidimension we would have

$$J_{adv} = a\chi\delta c$$

And so for us we get

$$J_{adv} = \chi a \frac{\partial c}{\partial x}$$

Where χ is a (constant) measure of strength of attraction to cAMP J_{adv} is called a **chemo-taxis** term (chemical movement \rightarrow movement up a chemical gradient). And χ is called the **chemotactic coefficient**.

So we get

$$\frac{\partial a}{\partial t} = \mu \frac{\partial^2 a}{\partial x^2} - \chi \frac{d}{dx} \left[a \frac{\partial c}{\partial x} \right]$$

But what about c ? We know that c is secreted by cells and diffuses freely in the environment

$$\frac{\partial c}{\partial t} = D \frac{\partial^2 c}{\partial x^2} + pa - kc$$

Where p is the production rate and k is the degradation rate (since degradation is proportional to its concentration)

So we have the system

$$\begin{aligned} \frac{\partial a}{\partial t} &= \mu \frac{\partial^2 a}{\partial x^2} - \chi \frac{\partial}{\partial x} \left(a \frac{\partial c}{\partial x} \right) \\ \frac{\partial c}{\partial t} &= D \frac{\partial^2 c}{\partial x^2} + pa - kc \end{aligned}$$

And introduce the boundary conditions

$$\frac{\partial a}{\partial x} = \frac{\partial c}{\partial x} = 0$$

At $x = 0, L$. I.e. there is no flux of cells or chemical at the boundaries of the confined region.

In terms of initial conditions, its a bit harder to say (and so we didn't say anything)

This is the Keller-Segel model of chemotaxis.

To non-dimensionalise the model, take

$$x = L\tilde{x}, \quad t = T\tilde{t}, \quad a = a_i\tilde{a}, \quad c = c^*\tilde{c}$$

Where a_i is the initial cell density and T, c^* are yet to be determined.

Plugging these in, dropping tildes, and rearranging gives

$$\begin{aligned} \frac{\partial a}{\partial t} &= \frac{\mu T}{L^2} \frac{\partial^2 a}{\partial x^2} - \frac{\chi T c^*}{L^2} \frac{\partial}{\partial x} \left(a \frac{\partial c}{\partial x} \right) \\ \frac{L^2}{TD} \frac{\partial c}{\partial t} &= \frac{\partial^2 c}{\partial x^2} + \frac{pa_i L^2}{Dc^*} a - \frac{kL^2}{D} c \end{aligned}$$

So take $T = L^2/\mu$ to get

$$\begin{aligned} \frac{\partial a}{\partial t} &= \frac{\partial^2 a}{\partial x^2} - \chi \frac{\partial}{\partial x} \left(a \frac{\partial c}{\partial x} \right) \\ \delta \frac{\partial c}{\partial t} &= \frac{\partial^2 c}{\partial x^2} + a - kc \end{aligned}$$

Where

- $\chi = \frac{pa_i \chi_{dimensional} L^2}{D\mu}$

- $k = \frac{k_{dimensional} L^2}{D}$
- $\delta = \frac{\mu}{D} (\ll 1)$ - since chemicals move more easily than cells.
- $c^* = \frac{pa_i L^2}{D}$

δ is a small parameter, and so we will look at **leading order solutions**, i.e. set $\delta = 0$.
With the BCs

$$\frac{\partial a}{\partial x} = \frac{\partial c}{\partial x} = 0, \quad x = 0, 1$$

6.3 Linear stability analysis

We want to know when and/or what conditions make the initially uniformly spread-out cells form aggregate.

Start with a **spatially uniform / spatially homogeneous steady state** of the model, i.e. a solution that is constant in space and time.

$$a(x, t) = \bar{a}, \quad c(x, t) = \bar{c}$$

We need to see if the equations allow this.

The first equation is trivially satisfied for constant \bar{a}, \bar{c} . The second equation gives

$$\bar{a} - k\bar{c} = 0, \quad \implies \quad \bar{c} = \frac{\bar{a}}{k}$$

This means that for a spatially homogeneous steady state to exist, the rate of chemical degradation must be exactly balanced by its rate of secretion by the cells.

See if the solution is stable or not - i.e. if a nearly uniform distribution of cells will stay that way, or if it is unstable, and we expect non-uniformities to grow in time.

Take a perturbation series

$$a = \bar{a} + \epsilon a_1(x, t) + \mathcal{O}(\epsilon^2), \quad c = \bar{c} + \epsilon c_1(x, t) + \mathcal{O}(\epsilon^2)$$

With $\epsilon \ll 1$.

Subbing into the equations gives:

$$\begin{aligned} \mathcal{O}(\epsilon) : \quad \frac{\partial a_1}{\partial t} &= \frac{\partial^2 a_1}{\partial x^2} - \chi \bar{a} \left(\frac{\partial^2 c_1}{\partial x^2} \right) \\ \frac{\partial^2 c_1}{\partial x^2} + a_1 - k c_1 &= 0 \end{aligned}$$

Use the ansatz $a_1, c_1 \propto e^{\lambda t} \cos qx$ where λ, q are tbd., but we know q is constrained by

$$\frac{\partial a}{\partial x} = \frac{\partial c}{\partial x} = 0, \quad x = 0, x = 1$$

This is why we ignored the sin term, but it also means that $q = n\pi$ for some integer n .

λ is the growth rate of the perturbation. Hence if $\lambda > 0$, the perturbation grows, and our spatially uniform solution is (linearly) unstable, if its negative then the spatially uniform solution is (linearly) stable.

So we have

$$\begin{aligned} a_1 &= A e^{\lambda t} \cos qx \\ c_1 &= C e^{\lambda t} \cos qx \end{aligned}$$

Plug into the equations (and simplify a little)

$$\begin{aligned}A\lambda &= -q^2 A + q^2 C \chi \bar{a} \\ -q^2 C + A - kC &= 0\end{aligned}$$

Which gives

$$\lambda = q^2 \left(\frac{\chi \bar{a}}{k + q^2} - 1 \right)$$

Noting that everything is real.

So if

$$\left| \frac{\chi \bar{a}}{k + q^2} \right| - 1 > 0$$

Then the solution is stable.

Recap: Necessary and sufficient conditions for instability

If we have

Condition X Holds \dots Instability occurs

- Necessary - gives the arrow pointing left (i.e. if instability occurs, then condition X holds) Instability is a subset of things where condition X holds. So

Condition X Holds \Leftarrow Instability occurs

- Sufficient - gives the arrow pointing right (i.e. if X holds, instability occurs) Condition X is a subset of instability.

Condition X Holds \Rightarrow Instability occurs

- Necessary and sufficient, double arrow, they are equal sets.

Condition X Holds \Leftrightarrow Instability occurs

So a necessary condition for $\lambda > 0$ here is

$$\left| \frac{\chi \bar{a}}{k + q^2} \right| - 1 > 0$$

Then the solution is stable.

We know $q^2 = n^2 \pi^2 \geq \pi^2$, $n \geq 1$ For this to be positive for any q , we need

$$\frac{\chi \bar{a}}{k + \pi^2} > 1$$

(Apparently χ , k and \bar{a} are positive)

What does this statement mean biologically? So we need χ, \bar{a} large and k small

Meaning we need:

- χ large - a strong chemotaxis effect relative to random motion of cells
- \bar{a} large - high cell density
- k small - the chemical cannot decay too quickly

Example: Travelling waves of haptotactic bacteria

Considering a colony of bacteria attracted to a nutrient they consume. If we have cell density b , and nutrient concentration c . The simple model in one dimension is

$$\begin{aligned}\frac{\partial b}{\partial t} &= D \frac{\partial^2 b}{\partial x^2} - \frac{\partial}{\partial x} \left(\chi \frac{b}{c} \frac{\partial c}{\partial x} \right) \\ \frac{\partial c}{\partial t} &= -kb\end{aligned}$$

Where D is the random diffusion coefficient of the bacteria, and k is the rate of nutrient consumption. The $\frac{\chi}{c}$ term is effectively the strength of attraction to nutrient.

Look for travelling wave solutions.

$$b(x, t) = B(z), \quad c(x, t) = C(z), \quad z = x - vt$$

Introduce boundary conditions

$$\begin{aligned}B &\rightarrow 0, \quad |z| \rightarrow \infty \\ C &\rightarrow 0 \quad \text{as } z \rightarrow -\infty, \quad C \rightarrow 1 \quad \text{as } z \rightarrow \infty\end{aligned}$$

Substituting into the system gives:

$$\begin{aligned}-v \frac{dB}{dz} &= D \frac{d^2 B}{dz^2} - \chi \frac{d}{dz} \left(\frac{B}{C} \frac{dC}{dz} \right) \\ -v \frac{dC}{dz} &= -kB\end{aligned}$$

Integrate the first equation once

$$-vB = D \frac{dB}{dz} - \chi \frac{B}{C} \frac{dC}{dz} + k_1$$

Using the BCs, $k_1 = 0$

$$-vB = D \frac{dB}{dz} - \chi \frac{B}{C} \frac{dC}{dz}$$

Using both equations we get

$$\begin{aligned}\frac{B'}{B} &= \frac{1}{D} \left(\chi \frac{C'}{C} - v \right) \\ C' &= \frac{kB}{v}\end{aligned}$$

Integrating both sides of the first gives

$$\log B = \frac{\chi}{D} \log C - \frac{v}{D} z + k_2$$

Special case, $\chi = 2D$ is analytic (skipping the steps) gives

$$\begin{aligned}B &= \frac{Kv^2}{Dk} \left(\frac{e^{-vz/D}}{(1 + Ke^{-vz/D})^2} \right) \\ C &= \frac{1}{1 + Ke^{-vz/D}}\end{aligned}$$

Where K is a constant.

For diffusion (spreading) we have

$$\frac{\partial n}{\partial t} = D \frac{\partial^2 n}{\partial x^2}$$

If we wanted reverse diffusion (aggregating), could we just write

$$\frac{\partial n}{\partial t} = -D \frac{\partial^2 n}{\partial x^2}?$$

We can't for a 'mathematically technical' reason.

The equation is the 'backwards heat equation', which we can't properly solve since we lose uniqueness of solutions. Plus, numerical error propagates when solving this.

A Hopf bifurcation occurs when the eigenvalues cross the imaginary axis. I.e. when the sign of the real part changes. You move from a stable steady state to an unstable steady state.

If you have $\lambda = \alpha \pm i\beta$

Then (if the equation has exponential solutions):

$$e^{\lambda t} = e^{\alpha t} (e^{i\beta t} + e^{-i\beta t})$$

And we can see α changing sign swaps from growth to decay (or vice-versa) with oscillatory behaviour.

The paper on swarms

$$\frac{\partial n}{\partial t} + \frac{\partial}{\partial x} (vn) = D \frac{\partial^2 n}{\partial x^2} + B(n)$$

Where $B(n)$ is some birth/death rate, but we will set it to zero for simplicity.

Most of the analysis comes from what the velocity, v looks like.

We want/expect to see 'clumping' of the individuals, kind of the opposite of diffusion/random motion.

These things will behave like boids. They want to clump together towards the centre of mass, but try not to get too close to each other... ideally.

As Ed put it, there are some pairwise attraction and repulsion effects between the individuals and their neighbours. Essentially there will be a force acting on individual A in the direction of B , and so on for all of the individuals. And so the movement of A will be the sum of these forces.

So if we were just looking at individuals in a discrete sense, we could just do this. But since we are using DEs, it must be continuous.

In continuous systems, a sum becomes an integral.

$$V(x) = \int_D K(x-y)n(y)dy$$

I.e. the convolution integral of K and the density function n over all y . K will be a function which describes the interaction between the point x and y . We will probably make it so that forces are positive (repulsive) for $|x-y| < d$ and then negative (attractive) past the distance d , up to some other distance d_{max} where it would go back to 0. K is called the kernel function. Note these variable names were made up by me so they will probably change.

We want $K(x)$ to be an odd function of x to account for directionality, so that individuals on opposite sides of an individual push/pull in opposite directions.

A different discussion: If we look at the KS model

$$\frac{\partial n}{\partial t} = D \frac{\partial^2 n}{\partial x^2} - \chi \frac{\partial}{\partial x} \left[n \frac{\partial c}{\partial x} \right]$$

$$\frac{\partial c}{\partial t} = D_c \frac{\partial^2 c}{\partial x^2} + pn - kc$$

An asymptotic approximation (after non-dimensionalisation) allows us to drop the $\frac{\partial c}{\partial t}$ term, giving (for the second equation)

$$\frac{\partial^2 c}{\partial x^2} - c = -n$$

Solve using Greens functions

$$\frac{\partial^2 c}{\partial x^2} - c = \delta(x - \zeta)$$

Where δ is a delta function

We would eventually get (for an infinite domain)

$$c(x, t) = \frac{1}{2} \int_{-\infty}^{\infty} n(y, t) e^{-|x-y|} dy$$

$$c_x(x, t) = -\frac{1}{2} \int_{-\infty}^{\infty} \text{sign}(x - y) n(y, t) e^{-|x-y|} dy$$

Which looks very similar to the $V(x)$ we had before. With kernel function

$$K(x - y) = -\frac{1}{2} \text{sign}(x - y) e^{-|x-y|}$$

This all relies on the infinite domain.

For locusts we have solitary and gregarious and we find that solitary ones can turn gregarious after enough interaction, and gregarious to solitary with enough alone time.

$$\frac{\partial s}{\partial t} + \frac{\partial}{\partial x}(v_s s) = -f_2(\rho)s + f_1(\rho)g$$

$$\frac{\partial g}{\partial t} + \frac{\partial}{\partial x}(v_g g) = f_2(\rho)s - f_1(\rho)g$$

We will let $v_s = k_s * \rho$, $v_g = k_g * \rho$ where $*$ means convolution integral. And where $\rho = s + g$ (total density). k_g will have attraction and repulsion, while k_s only has repulsion. f_2 is the rate of movement from solitary to gregarious, and f_1 is the rate of movement from gregarious to solitary. The locusts can't tell if other locusts are gregarious or solitary. Look at a linear stability analysis.

7 Turing Patterns

Morphogenesis - the creation of patterns in biology

Say you have a patch of tissue with some chemicals (we will say two chemicals) which diffuse and react.

The patch of cells will do something in response to the concentration of the chemicals

If the chemicals are A and B

$$\begin{aligned} \frac{\partial A}{\partial t} &= D_A \nabla^2 A + F(A, B) \\ \frac{\partial B}{\partial t} &= D_B \nabla^2 A + G(A, B) \end{aligned}$$

We need F, G to be nonlinear for any interesting dynamics.

Boundary conditions, no flux at edges of the tissue

$$\hat{n} \cdot \nabla A = \hat{n} \cdot \nabla B = 0, \text{ on the boundary}$$

Of course we will also need an initial condition for A, B .

A, B are morphogens - they cause the morphogenesis

Because we hate numbers greater than 1, we will assume $1D$.

Non-dimensionalisation gives:

$$\begin{aligned}\frac{\partial a}{\partial t} &= \frac{\partial^2 a}{\partial x^2} + \gamma f(a, b) \\ \frac{\partial b}{\partial t} &= d \frac{\partial^2 b}{\partial x^2} + \gamma g(a, b)\end{aligned}$$

Where γ is related to the domain length, d is the ratio D_B/D_A

Solve on the domain $0 \leq x \leq L$.

Look at the spatially uniform steady state, and then perturb

Assume that state exists for

$$(a, b) = (a_0, b_0) > 0$$

(they have to be zeroes of f, g)

In the absence of diffusion

$$\begin{aligned}\frac{\partial a}{\partial t} &= \gamma f(a, b) \\ \frac{\partial b}{\partial t} &= \gamma g(a, b)\end{aligned}$$

Small perturbations to the spatially uniform steady state

$$\begin{aligned}a &= a_0 + \epsilon a_1 + \mathcal{O}(\epsilon^2) \\ b &= b_0 + \epsilon b_1 + \mathcal{O}(\epsilon^2)\end{aligned}$$

Where $\epsilon \ll 1$.

Can write the system (at first order) as

$$\frac{\partial}{\partial t} \begin{pmatrix} a \\ b \end{pmatrix} = \gamma \begin{pmatrix} f_a & f_b \\ g_a & g_b \end{pmatrix} \begin{pmatrix} a_1 \\ b_1 \end{pmatrix}$$

Where f_a, f_b, g_a, g_b are partial derivatives, evaluated at a_0, b_0 . Can rewrite as

$$\frac{\partial \mathbf{w}}{\partial t} = \gamma M \mathbf{w}$$

Where $w = (a_1, b_1)^T$ and M was the matrix from before.

For the fixed point/steady state a_0, b_0 to be stable, require eigenvalue of M to give stability.

So we require

$$\begin{aligned}tr(M) &= f_a + g_b < 0 \\ det(M) &= f_a g_b - f_b g_a > 0\end{aligned}$$

Now assuming those equations hold, it is stable. But if we include the diffusion terms it gets more interesting. We can write it as

$$\frac{\partial \mathbf{w}}{\partial t} = D \frac{\partial^2 \mathbf{w}}{\partial x^2} + \gamma M \mathbf{w}$$

Where

$$D = \begin{pmatrix} 1 & 0 \\ 0 & d \end{pmatrix}$$

From earlier solutions, we expect

$$\mathbf{w} \propto e^{\lambda t} \cos(qx)$$

And since we want no flux on $x = L$ we have $q = \frac{n\pi}{L}$

We just need to find an unstable \mathbf{w} . Substitute into \mathbf{w} :

$$\lambda \mathbf{w} = -q^2 D \mathbf{w} + \gamma M \mathbf{w}$$

For non-trivial solutions,

$$\det [\lambda I + q^2 D - \gamma M] = 0$$

Which ends up giving

$$\lambda^2 + \lambda[q^2(1+d) - \gamma(f_a + g_b)] + h(q^2) = 0$$

Where

$$h(q^2) = dq^4 - \gamma(df_a + g_b)q^2 + \gamma^2 \det(M)$$

The steady state (a_0, b_0) will be linearly stable if both roots have $Re(\lambda) < 0$. From before we found that for $q = 0$, then it holds.

Want to show that there is a $q \neq 0$ which gives $Re(\lambda) > 0$. From the quadratic formula we get

$$\begin{aligned} ax^2 + bx + c &= 0 \\ (x_0 + x_1) &= -b \\ x_0 x_1 &= c \end{aligned}$$

Where x_0, x_1 are the roots.

So for our quadratic we will have at least one root with $Re(\lambda) > 0$ if either:

$$\begin{aligned} h(q^2) &< 0 \\ q^2(1+d) - \gamma(f_a + g_b) &< 0 \end{aligned}$$

The second

$$q^2(1+d) - \gamma(f_a + g_b) < 0$$

We know the first term is positive since $q^2 > 0$ and $d > 0$ (no negative diffusion). For the second term however, we assumed $tr(M) < 0$, and $\gamma > 0$ since it relates to domain length. So this inequality does not hold.

The other equation

$$\begin{aligned} h(q^2) &< 0 \\ dq^4 - \gamma(df_a + g_b)q^2 + \gamma^2 \det M &< 0 \end{aligned}$$

The first term is always positive, the last term is positive by our earlier assumption. So a necessary condition is $df_a + g_b > 0$ (it is most certainly not sufficient). And so we need f_a, g_b to have opposite signs, and $d \neq 1$.

For $h(q^2)$ to be negative, for some $q \neq 0$, then obviously its minimum value must be negative. Let q_c be the value of q that obtains the minimum, i.e. $h(q_c^2) = h_{min}$.

At the min $\frac{dh}{dq^2} = 0$

$$2dq^2 - \gamma(df_a + g_b) = 0$$

$$q^2 = \frac{\gamma(df_a + gb)}{2d}$$

And so

$$h_{min} = \gamma^2 \left(\det M - \frac{(df_a + gb)^2}{4d} \right)$$

For instability, this has to be negative, and hence

$$\det M - \frac{(df_a + gb)^2}{4d} < 0$$

$$\det M < \frac{(df_a + gb)^2}{4d}$$

So there is a bifurcation from stable to unstable when $h_{min} = 0$. Which defines a critical diffusion ratio, d_c (assuming f, g are given). It satisfies

$$d_c^2 f_a^2 + 2(2f_b g_a - f_a g_b) d_c + g_b^2 = 0$$

For $d < d_c$, there are no unstable wavenumbers. For $d > d_c$ then we expect at least one unstable wavenumber.

For $d > d_c$, look at h :

$$h(q^2) = dq^4 - \gamma(df_a + g_b)q^2 + \gamma^2 \det M$$

As $q^2 \rightarrow \infty$, $h(q^2) \rightarrow dq^4$, so large wavenumbers are stable, we already know $q = 0$ is stable. So instability occurs for some range of $0 < q_1 < q < q_2$. Note that q_1, q_2 will be roots of h , i.e. $h(q_1^2) = h(q_2^2) = 0$.

To satisfy all the boundary conditions, we require $q = n\pi/L$.

So the perturbed solutions will have form

$$(a_1, b_1) = \sum_{q_n} (\alpha_n, \beta_n) e^{\lambda_n(q_n^2)t} \cos q_n x$$

For the values of q which give negative λ_n , those terms decay quickly. The unstable ones will grow and will dominate. We expect that those q_n which give the largest λ_n will dominate the others, and will be the fastest growing node(s), the dominating pattern.

Note that when these have grown large enough, the perturbation ansatz falls apart and a full analysis must be done.

Note that we never obtained sufficient conditions, but the list of necessary conditions for the diffusion-driven instability is:

$$f_a + g_b < 0 \tag{1}$$

$$f_a g_b - f_b g_a > 0 \tag{2}$$

$$df_a + g_b > 0 \tag{3}$$

$$(df_a + g_b)^2 - 4d(f_a g_b - f_b g_a) > 0 \tag{4}$$

Where all f_a, g_b are evaluated at a_0, b_0 .

What is the physical explanation/interpretation of this?

- (1) : at least one of f_a, g_b is negative. Lets assume its g_b . Then b inhibits its own rate of formation (it is an **inhibitor**).
- (3) : if $g_b < 0$, then $f_a > 0$. So a promotes its own rate of formation (it is an **activator**)
- Hence we have $f_a g_b < 0$, and so (2) requires $f_b g_a < 0$. This means that either $f_b < 0$ or $g_a < 0$, and the other is positive. The signs of the values in the matrix make the difference:

$$M = \begin{pmatrix} f_a & f_b \\ g_a & g_b \end{pmatrix}$$

Then there are two possibilities:

– Activator-inhibitor

$$f_b < 0, \quad g_a > 0, \quad M = \begin{pmatrix} + & - \\ + & - \end{pmatrix}$$

– Positive-feedback

$$f_b < 0, \quad g_a > 0, \quad M = \begin{pmatrix} + & + \\ - & - \end{pmatrix}$$

- Looking at (1), (3), we require $d \neq 1$. We require $d > 1$ to satisfy (3) (since we have chosen $f_a > 0, g_b < 0$).
- Inhibitor diffuses faster than the activator since $d = \frac{D_B}{D_A}$.

If we specifically look at the Activator-inhibitor case, i.e. where a is the activator, b the inhibitor.

If we plot a, b against space x , and we perturb from the steady state solution (a_0, b_0) . A build up of a will cause a build up of b . b inhibits a , and then both would then decrease. Since the diffusion is present, we find b diffuses more through space. Hence you don't build up enough b in one place to control the amount of a , so a continues to grow at the peak. Essentially there will only be the one peak of a , with quite high concentration. The 'shoulders' of the peak are controlled nicely by b , so we only see the highest wavenumber peak(s).

Reminder of the system

$$\begin{aligned} \frac{\partial a}{\partial t} &= \frac{\partial^2 a}{\partial x^2} + f(a, b) \\ \frac{\partial b}{\partial t} &= d \frac{\partial^2 b}{\partial x^2} + g(a, b) \end{aligned}$$

Need to assume a steady state, (a_0, b_0) .

A random question given

$$\frac{\partial U}{\partial t} = rU \left(1 - \frac{U}{K}\right) - EU + D \frac{\partial^2 U}{\partial x^2}$$

Change wrt time is the logistic reproduction the consumption and the diffusion.

$$U = 0, x = 0, \quad \frac{\partial U}{\partial x} = 0, \quad x = 0$$

Spatially uniform ss means $\frac{\partial U}{\partial x} = 0$ and $\frac{\partial U}{\partial t} = 0$

$$\begin{aligned} 0 &= rU(1 - \frac{U}{K}) - EU \\ r(1 - \frac{U}{K}) - E &= 0 \\ \frac{E}{r} &= 1 - \frac{U}{K} \\ U &= K(1 - \frac{E}{r}), \quad 0 \end{aligned}$$

Linear stability,
We will have

$$U = \epsilon \cos(qx)e^{\lambda t}$$

Sub in

$$\begin{aligned} \frac{\partial U}{\partial t} &= rU(1 - \frac{U}{K}) - EU + D \frac{\partial^2 U}{\partial x^2} \\ \lambda \epsilon \cos(qx)e^{\lambda t} &= r(\epsilon \cos(qx)e^{\lambda t}) \left(1 - \frac{\epsilon \cos(qx)e^{\lambda t}}{K}\right) - E(\epsilon \cos(qx)e^{\lambda t}) - Dq^2 \epsilon \cos(qx)e^{\lambda t} \end{aligned}$$

Like powers of ϵ

$$\lambda = r - E - Dq^2$$

This is the dispersion relation. I.e. the sign of the real part of λ .
using the BCs

$$\begin{aligned} q &= \frac{(2n+1)\pi}{H} \\ \lambda &= r - E - D \left(\frac{(2n+1)\pi}{H} \right)^2 \end{aligned}$$

Assuming $\lambda \in \mathbb{R}$
Unstable if $\lambda > 0$.

$$\lambda > 0 \implies r - E - Dq^2 > 0$$

$$q^2 = \left(\frac{(2n+1)\pi}{H} \right)^2 < \frac{r - E}{D}$$

We can take the minimum n for this

$$\begin{aligned} \left(\frac{\pi}{2H} \right)^2 &< \frac{r - E}{D} \\ H &> \frac{\pi}{2} \left(\frac{D}{r - E} \right)^{1/2} \end{aligned}$$

So that the fishing population doesn't collapse i.e. we don't hit the trivial steady state, we require these unstable states! So if the domain H is larger than this threshold, the fish are given the chance to reproduce, and the population is kept up.

$$\begin{aligned}\frac{\partial u}{\partial t} &= a - u + u^2v + \frac{\partial^2 u}{\partial x^2} \\ \frac{\partial v}{\partial t} &= 3a - u^2v + d\frac{\partial^2 v}{\partial x^2}\end{aligned}$$

$d, a > 0$ are constants and $0 \leq x \leq L$.

$$\frac{\partial u}{\partial x} = \frac{\partial v}{\partial x} = 0, \quad x = 0, L$$

Steady state:

$$\begin{aligned}0 &= a - u + u^2v + \frac{\partial^2 u}{\partial x^2} \\ 0 &= 3a - u^2v + d\frac{\partial^2 v}{\partial x^2}\end{aligned}$$

8 Growing Tissues

8.1 Modelling Avascular Tumours

An avascular tumour is the most simple form of tumour. An avascular tumour does not have its own blood supply (no blood vessels) - it is an early stage tumour. They tend to be quite small since they do not get any supply of oxygen or nutrient via any means other than diffusion. Hence it cannot grow any more until it becomes **vascularised** (it gains a system of blood vessels). Expect cells in the middle to become necrotic (dead) when they no longer get nutrient. Outside of this we expect quiescent cells - they aren't quite getting enough nutrient to proliferate, but they have enough to be alive. The outermost ring will have the proliferative cells. Often not worth distinguishing the quiescent cells. Just considering alive and dead cells.

For simplicity, consider a spherical tumour with radial coordinate r . Let the radius of the necrotic core be a (when it exists) and the radius of the tumour be R . R and a are functions of t . Assume there is a single nutrient which is vital to the cells' life, with concentration c . Live cells will consume the nutrient at constant rate k , while necrotic cells will not, so we have different equations in the two regions. Assume that diffusion of the nutrient occurs on a shorter timescale than that of tumour growth, and that nutrient transport is only by diffusion in the tumour. The short timescale means we will take a quasi-steady assumption.

This is a free boundary problem since the domain for c includes a and R .

Assuming the nutrient diffuses equally through both regions, the model equations are:

$$\begin{aligned}\frac{\partial c}{\partial t} &= D\nabla^2 c, \quad 0 < r < a \\ \frac{\partial c}{\partial t} &= D\nabla^2 c - k, \quad a < r < R\end{aligned}$$

And then using the quasi-steady assumption, and using spherical polar coordinates

$$\begin{aligned}0 &= D\frac{1}{r^2}\frac{\partial}{\partial r}\left(r^2\frac{\partial c}{\partial r}\right), & 0 < r < a \\ 0 &= D\frac{1}{r^2}\frac{\partial}{\partial r}\left(r^2\frac{\partial c}{\partial r}\right) - k, & a < r < R\end{aligned}$$

Boundary conditions: Outside the tumour, assume that nutrient concentration is constant

$$c = c^*, \quad \text{on } r = R$$

If the nutrient concentration drops below some critical value c_n , cells become necrotic

$$c(a) = c_n$$

In the early stages of growth, the tumour is too small for necrotic core to develop ($a = 0$). So in this domain the system reduces to the single equation

$$0 = D \frac{1}{r^2} \frac{\partial}{\partial r} \left(r^2 \frac{\partial c}{\partial r} \right) - k, \quad c(R) = c^*$$

We also require non-singular solutions at the origin $r = 0$, which gives us another bc.

Solving this gives

$$c(r) = \frac{k}{6D} r^2 + \frac{A}{r} + B$$

Where A, B are constants. Clearly $A = 0$ to remove the singularity at $r = 0$, Imposing $c(R) = c^*$ gives

$$c(r) = c^* - \frac{k}{6D} (R^2 - r^2)$$

This is only valid for $c_{min} > c_n$. Minimum c occurs at $r = 0$. So we require

$$c(0) = c^* - \frac{kR^2}{6D} > c_n$$

$$R^2 < R_c^2 = \frac{6D(c^* + c_n)}{k}$$

So there is a critical value when:

$$c^* - \frac{kR_c^2}{6D} = c_n$$

When the tumour has a necrotic core, have to use the full system. $R > R_c$

$$\begin{aligned} \frac{\partial c}{\partial t} &= D \nabla^2 c, \quad 0 < r < a \\ \frac{\partial c}{\partial t} &= D \nabla^2 c - k, \quad a < r < R \end{aligned}$$

Need to solve the pair of equations such that at the boundary $r = a$ the system is continuous.

I.e. require both c and $-D \frac{\partial c}{\partial r}$ are continuous.

In $0 < r < a$

$$c = Ar + B$$

But for $a \neq 0$ we have $A = 0$ (else we would get singularities at $r = 0$), and hence we get

$$c = c_n, \quad 0 < r < a$$

Hence at $r = a$ the nutrient flux is zero.

In $a < r < R$, we have

$$c = \frac{k}{6D} r^2 + \frac{A}{r} + B$$

We have three unknowns, A, B, a

Conditions:

$$\begin{aligned} c(a) &= c_n \\ -D \frac{\partial c}{\partial r} \Big|_{r=a} &= 0 \\ c(R) &= c^* \end{aligned}$$

$$\begin{aligned} \frac{k}{6D}a^2 + \frac{A}{a} + B &= c_n \\ \frac{ka}{3D} - \frac{A}{a^2} &= 0 \\ \frac{kR^2}{6D} + \frac{A}{R} + B &= c^* \end{aligned}$$

Using the second gives us

$$A = \frac{ka^3}{3D}$$

Subtracting the third from the first gives

$$\begin{aligned} \frac{k}{6D} (a^2 - R^2) + A \left(\frac{1}{a} + \frac{1}{R} \right) &= c^* - c_n \\ \frac{k}{6D} \left[R^2 - a^2 - 2a^3 \left(\frac{1}{a} - \frac{1}{R} \right) \right] &= c^* - c_n \\ \frac{kR^2}{6D} \left(1 + \frac{2a}{R} \right) \left(1 - \frac{a}{R} \right)^2 &= c^* - c_n \\ \frac{k}{6D} \left(1 + \frac{2a}{R} \right) (R - a)^2 &= c^* - c_n \end{aligned}$$

As $R \rightarrow \infty$ the third equation gives us $\frac{a}{R} \rightarrow 1$. Which means $a \rightarrow \infty$ Let $h = R - a$ (the width of the proliferative part) The last equation says that $h^2 \rightarrow \frac{2D(c^* - c_n)}{k}$ as $R \rightarrow \infty$

Of course we don't actually have any information about how the tumour is growing, and how a, R grow with time. Previously we considered a, R as parameters, but now we will consider this as a full model for the evolution of $R(t), a(t)$.

- Let n be the density of tumour cells.
- Let v be the radial velocity of tumour cells
- No proliferation in the necrotic core
- Cells in the necrotic core break down at rate β
- In the live region, $a < r < R$ the cells are proliferating
- Assume rate of proliferation is constant γ when $c > c_n$
- Assume density is a uniform constant, and w.l.o.g. it is 1.

Conservation should be of form (since we are using spherical coordinates)

$$\begin{aligned}\frac{\partial n}{\partial t} + \frac{1}{r^2} \frac{\partial}{\partial r}(r^2 n v) &= -\beta n, & 0 < r < a \\ \frac{\partial n}{\partial t} + \frac{1}{r^2} \frac{\partial}{\partial r}(r^2 n v) &= \gamma n, & a < r < R\end{aligned}$$

Our assumption of constant $n = 1$ reduces the system to

$$\begin{aligned}\frac{1}{r^2} \frac{\partial}{\partial r}(r^2 v) &= -\beta, & 0 < r < a \\ \frac{1}{r^2} \frac{\partial}{\partial r}(r^2 v) &= \gamma, & a < r < R\end{aligned}$$

With a requirement of the continuity of velocity at $r = a$.

Solving the system gives

$$\begin{aligned}v &= -\frac{1}{3}\beta r, & 0 < r < a(t) \\ v &= \frac{1}{3}\gamma r - \frac{1}{3}(\beta + \gamma) \frac{a^3}{r^2}, & a(t) < r < R(t)\end{aligned}$$

We wanted an equation for R though, noting that the velocity at R is the cell velocity at $r = R(t)$ I.e.

$$\begin{aligned}\frac{\partial R}{\partial t} &= v(R(t), t) \\ \frac{\partial R}{\partial t} &= \frac{1}{3}\gamma R - \frac{1}{3}(\beta + \gamma) \frac{a^3}{R^2} \\ \frac{\partial R}{\partial t} &= \frac{1}{3}\gamma R \left[1 - \frac{(\beta + \gamma)}{\gamma} \left(\frac{a^3}{R^3} \right) \right]\end{aligned}$$

We already have an equation for a in terms of R . The unfortunate thing is the equation is a ‘nasty mess’.

Often $\beta \ll \gamma$, so let $\epsilon = \frac{\beta}{\gamma} \ll 1$, so we expect the tumour to grow large with a large necrotic core. We expect $\frac{h}{R}$ to be small.

A steady state exists for

$$\begin{aligned}1 - \frac{\beta + \gamma}{\gamma} \left(\frac{a^3}{R^3} \right) &= 0 \\ (1 + \epsilon) \left(\frac{a^3}{R^3} \right) &= 1 \\ \frac{1}{1 + \epsilon} &= \frac{a^3}{R^3} \\ \frac{1}{1 + \epsilon} &= \frac{(R - h)^3}{R^3} \\ \frac{1}{1 + \epsilon} &= \left(1 - \frac{h}{R} \right)^3 \\ 1 - \epsilon + \mathcal{O}(\epsilon)^2 &= 1 - 3\frac{h}{R} + \mathcal{O}\left(\frac{h}{R}\right)^2\end{aligned}$$

So

$$3\frac{h}{R} \simeq \epsilon \implies R \simeq \frac{3h\gamma}{\beta}$$

End of examinable content
 In divergence equations e.g.

$$\nabla \cdot (\mathbf{u}) = S$$

If \mathbf{u} is multidimensional (non-symmetric in those dimensions), we need a ‘Constitutive law’.
 In this case, Darcy’s Law for a porous medium:

$$\mathbf{u} = -\mu \nabla p$$

(μ is porosity and p is the pressure).

$$\frac{\partial a}{\partial t} = \nabla \cdot (const \nabla a) - \frac{\partial b}{\partial t} = const \nabla a \frac{\partial f}{\partial t} = \lambda_0 - \alpha a g(f) - \beta b h(f) + \frac{\partial}{\partial x} \left(D \frac{\partial f}{\partial x} \right)$$

$g(f)$ and $h(f)$ have to be linear(ish) initially and plateau later, an example is

$$\frac{f}{\alpha_1 + f}$$