

# System Identification and Control of Anatomically Accurate Biomechanical Human Limb Models

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## Background

Previous studies suggest that the neural responses in the motor cortex may be encoding:

- 1. High level parameters such as elbow position.
- 2. Low level parameters such as muscle activity.
- 3. Patterns of **goal driven models**, such as PIDs trained to output signals to excite muscles [1], [2].

However, the limitations of these models include:

- 1. Do not consider anatomically correct models [3].
- 2. Do not consider the **complex underpinnings of musculoskeletal dynamics** such as non-linear muscle actuators.
- 3. Require **experimentally recorded data**, such as muscle activity, for training.
- 4. Cannot predict motor cortex neural responses during unobserved conditions, since they do not generalize well to changes in environment and perturbation analyses.
- 5. Do not elucidate the role of the motor cortex as a controller for the musculoskeletal dynamics [4].

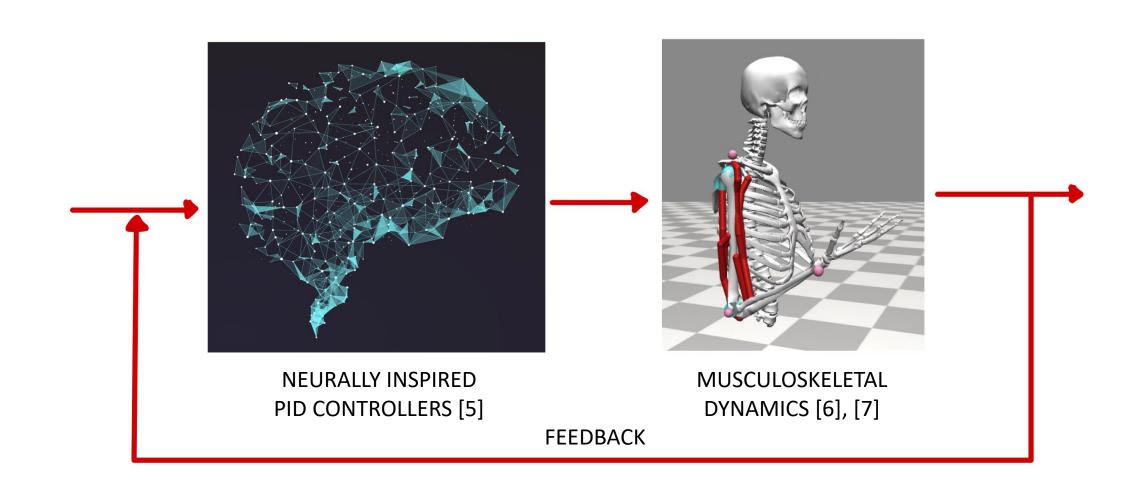


Fig. 2: Proposed Internal Model of Sensorimotor Control Loop

# Summary

We developed a simulation framework to model the cerebrocerebellar neural dynamics of the motor cortex as a set of time-invariant PID controllers. We trained the controllers on a **10**<sup>th</sup> **order linear dynamical system** which acted as a linear approximation of the nonlinear musculoskeletal dynamics of the OpenSim model. We observed that:

- 1. The system performed well on the training data but **performed poorly on held-out data**. It may not have identified the dynamics properly.
- 2. The **step response was blazing fast** with a rise time of 0.009 seconds, a settling time of 0.047 seconds, and an overshoot of 18.7327%. This allowed the gain settings to be decreased significantly in manual tuning to allow the plant to track the reference with good quality.
- 3. Tracking only the elbow joint appears to cause oscillatory behavior for the shoulder joint.

# **Trajectory Tracking Performance**

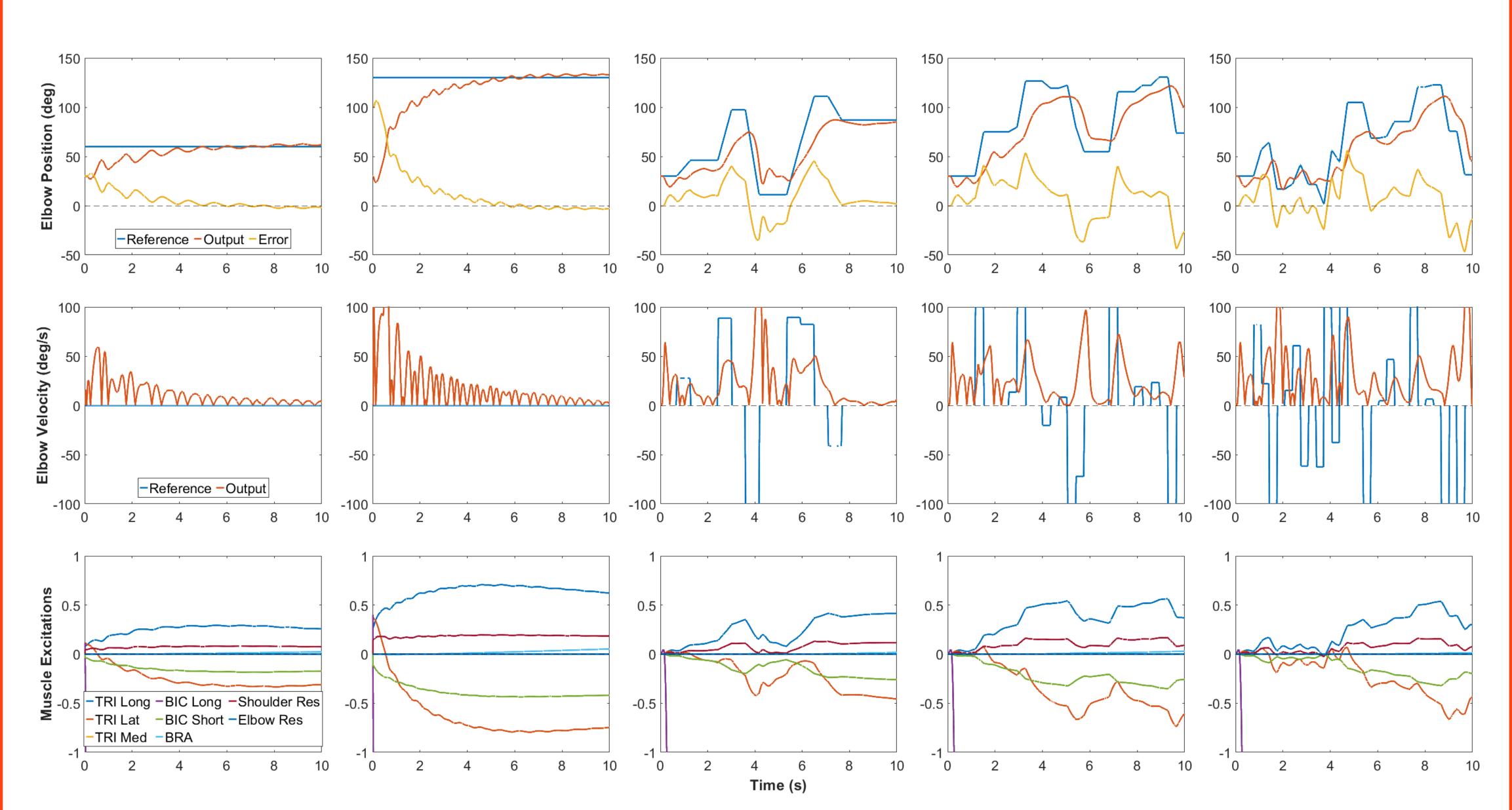


Fig. 1: Reference Tracking Performance of the System. Elbow Position and Velocity and the resulting Muscle Excitations are Displayed.

## **Methods and Technical Details**

#### **System Identification**

- 5000 motions for training with 500 for validation.
- Eight inputs (muscle activations) and two outputs (elbow joint angular position and speed).
- Estimated linear dynamical systems of order 2 to 15.

#### **Control Loop**

- Designed a PID controller to each muscle input to drive the system towards a reference input.
- Tested the tracking performance of complex signals and step signals using a discretized control loop and an application to control the system.

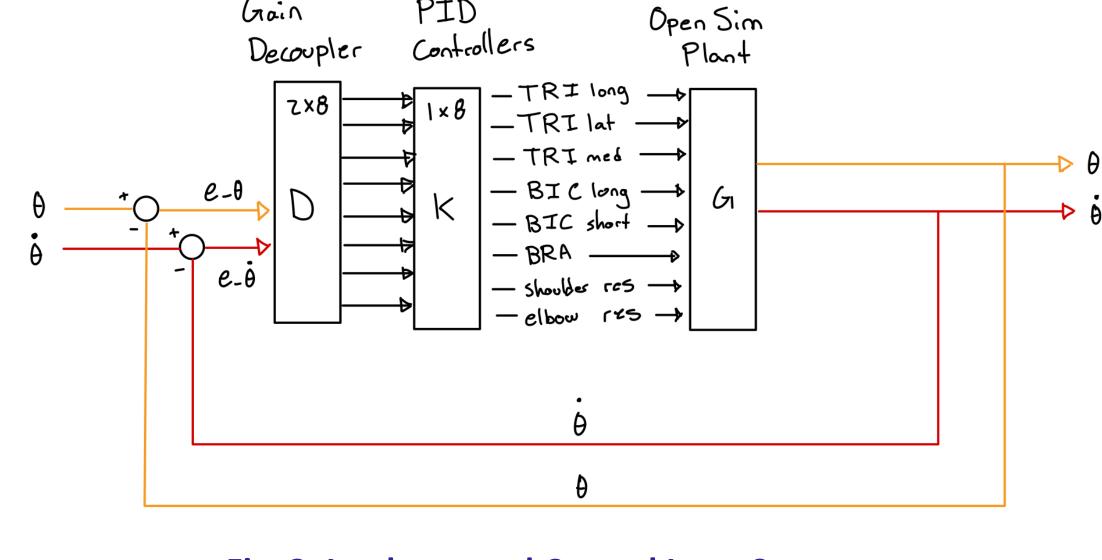


Fig. 3: Implemented Control Loop Structure

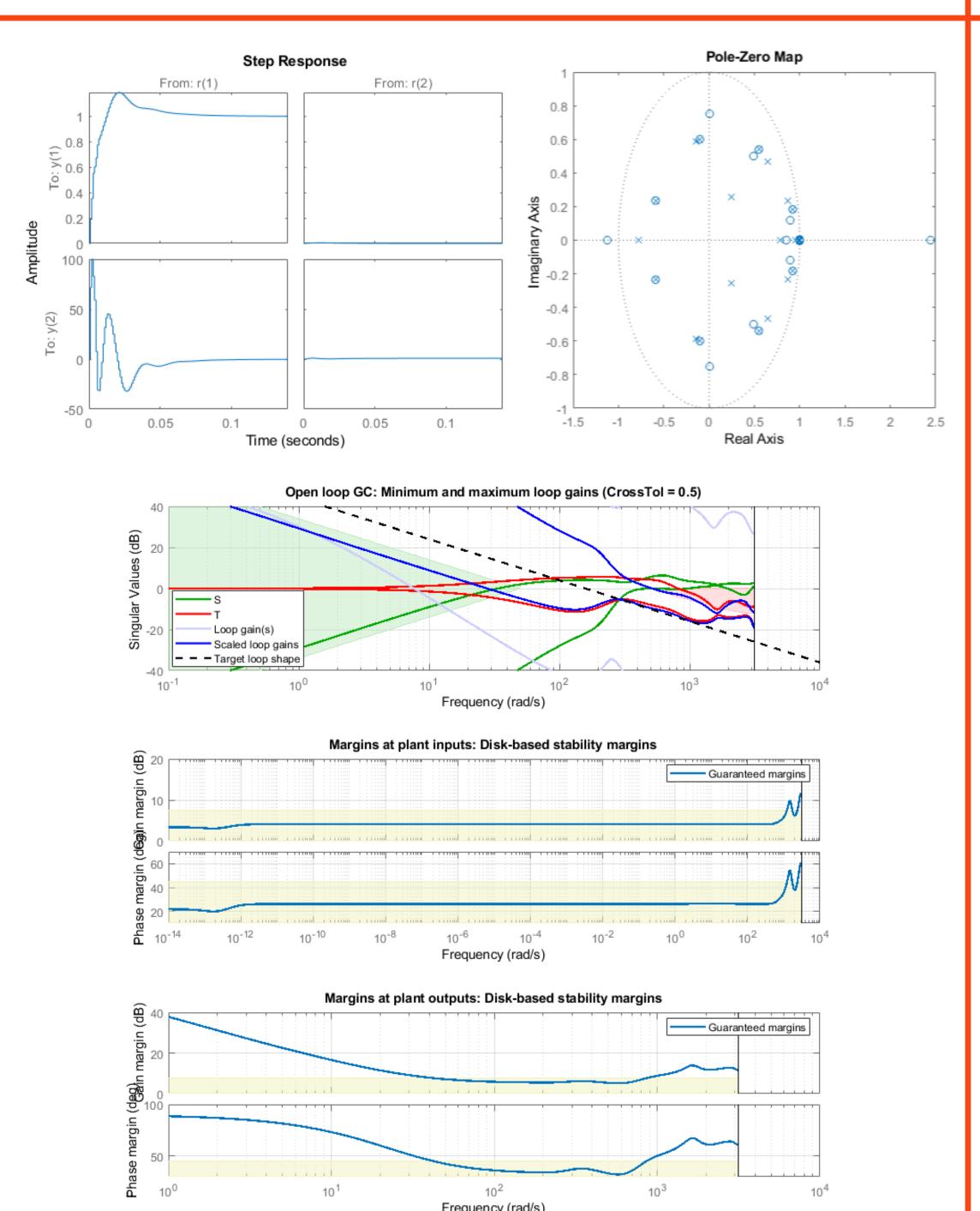


Fig. 4-6: (4) Step Response, (5) Pole-Zero Map, and (6) Frequency-Domain Response of the 10<sup>th</sup> Order System.

## System Identification

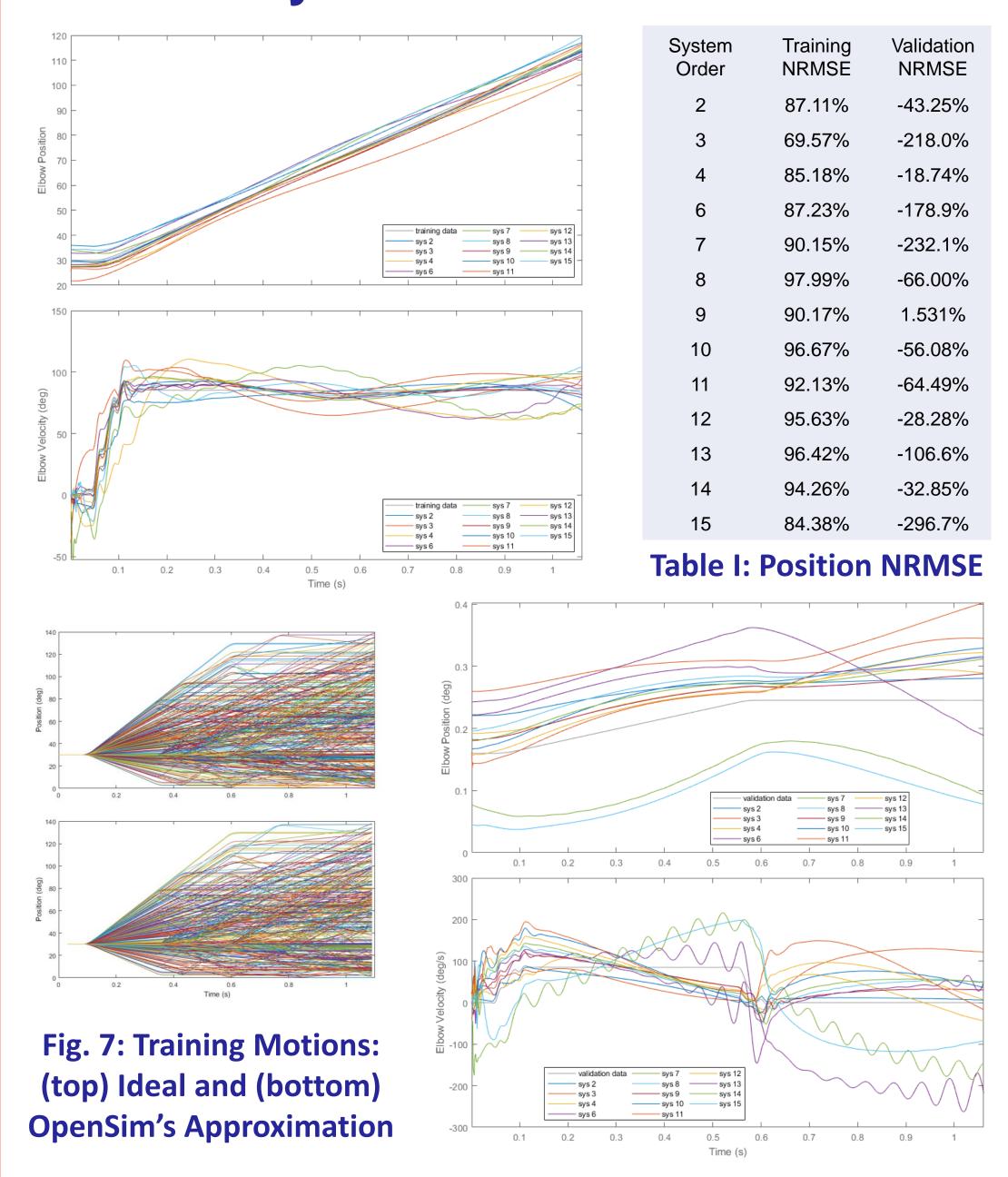


Fig. 8-9: Comparison of Each System Order with the (8) Training Data and (9) Validation Data. A System of Order 10 was Chosen.

# **Future Directions**

- 1. Improve reference tracking ability of the controllers through retraining on better data sets, addition of derivative component in the designed controllers, and or modeling biophysical bounds in the cerebrocerebellar dynamics.
- 2. Pursue the design of assistive neuroprosthetic devices which implement controllers to add compensatory forces to restore motor neural dynamics compromised by damage or disease [8].
- 3. Expanding the neural dynamics to include a spiking model of the efferent alpha motor neurons as they excite motor unit recruitment [8].
- 4. Expanding the musculoskeletal dynamics to include the ability to track the shoulder joint and to track the wrist and fingers.

### References

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[2] S. Saxena, et al., bioRxiv (2021).

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