

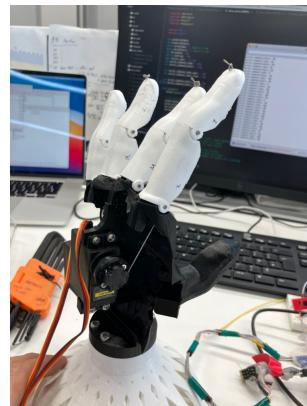
WORKSHOP 6

Human-Machine Interfacing and Mechatronics for Myoelectric Prosthetics

Goal: Explore from designing a bionic limb, assembling it, and implement a control system to control using sEMG

1st Day

Build your bionic limb



Lecture content (~20 min):

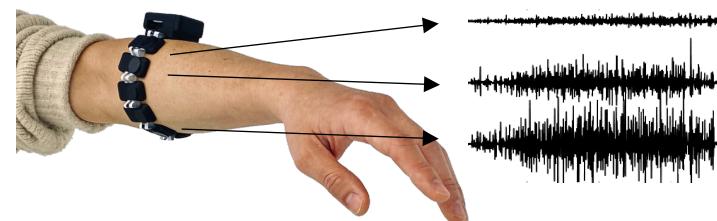
- Generics on Bionic Limb reconstruction

Task (~1h 30 min):

- CAD (get an idea on how to design a bionic limb)
- Assemble simplified limb
- Actuate the hand by a code command

2nd Day

Muscle interfacing techniques



Lecture content (~30 min):

- Fundamental signal for motor control
- Interfacing with the Nervous system
- Feature extraction
- Data driven prosthesis control

Task (~1h 30 min):

- Implement an algorithm to create a 2DOF regressor

3rd Day

Integration into online bionic limb control



Task1 (~45min):

- Online interfacing by using a neural interface device
- Exploration on different gestures and labels

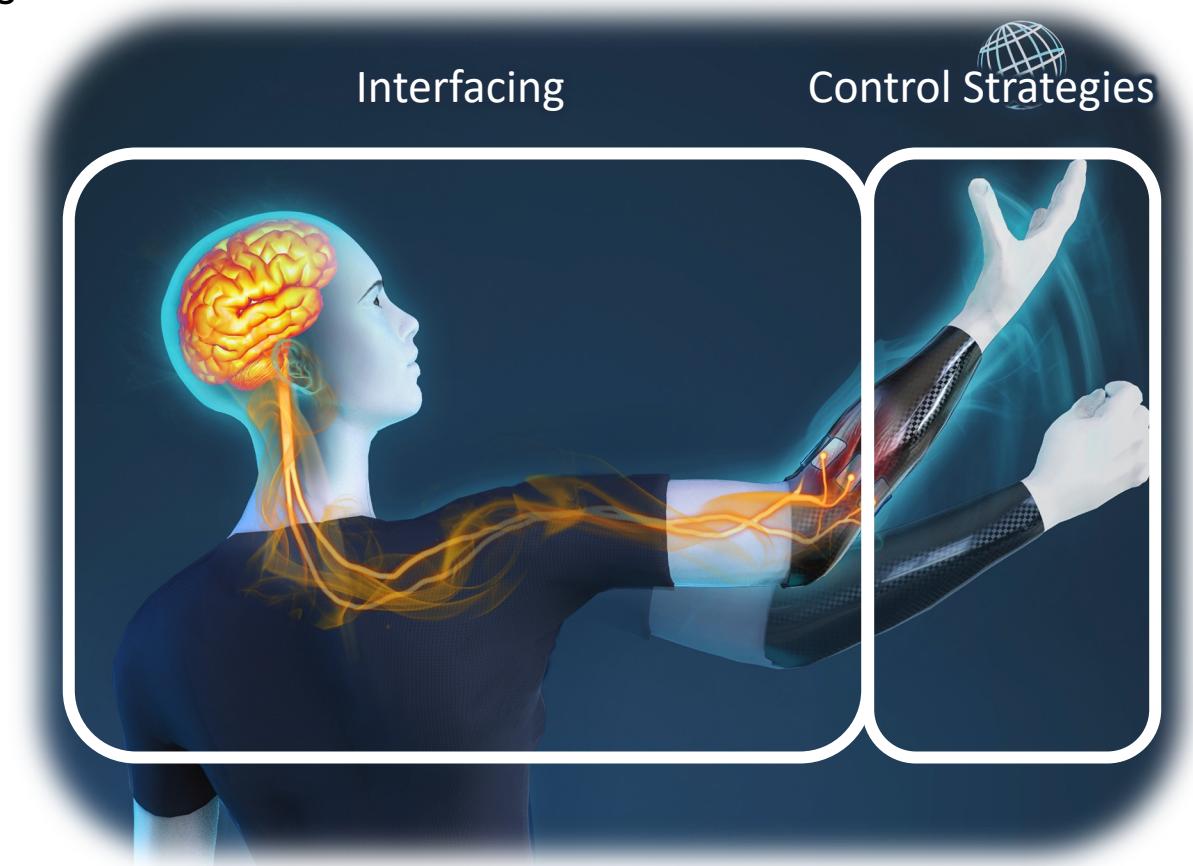
Task2 (~45min):

- Connect to a bionic hand and control by using your own muscle signals

Wrap up and Q&A (30min)

Controlling prosthesis by BCI

- ❖ Interfacing and control are the remaining challenges



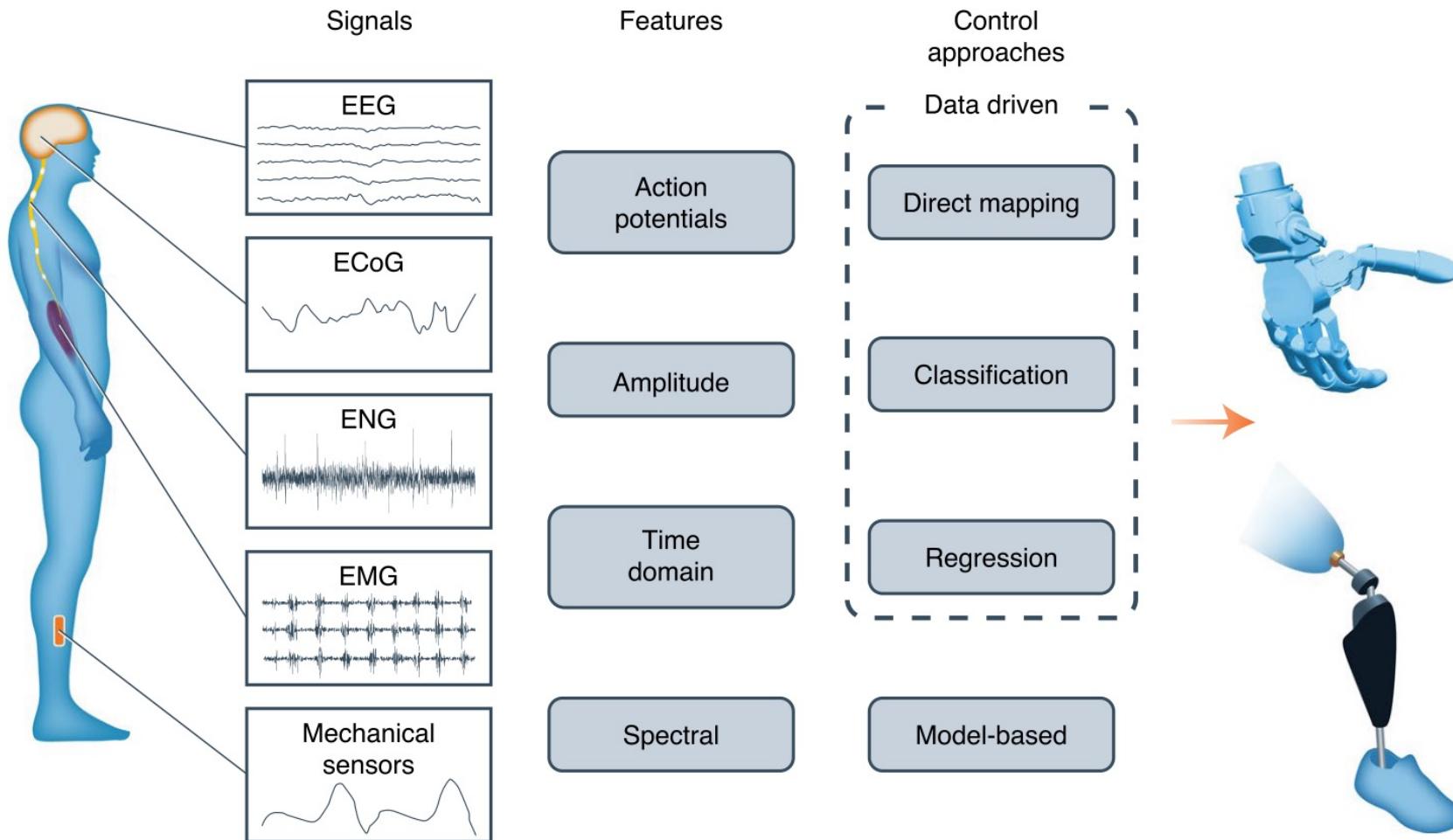
Mechanics on prosthesis are well matured, but the interfacing to human's neural system and the control strategies are yet to meet the user fulfillment

Interfacing



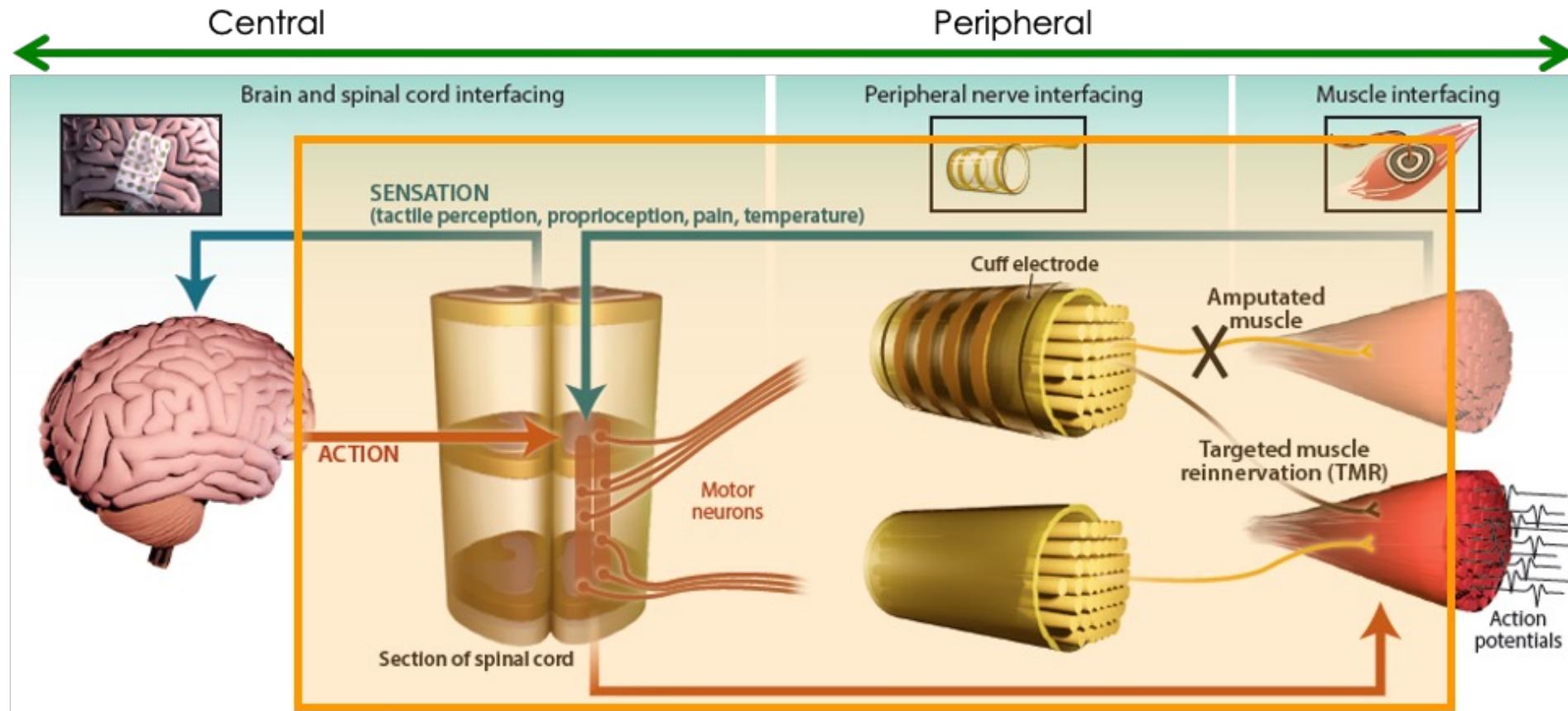
Controlling prosthesis by BCI

- ❖ Multiple ways to interface biological signals and control assistive devices



Muscle is a biological amplifier

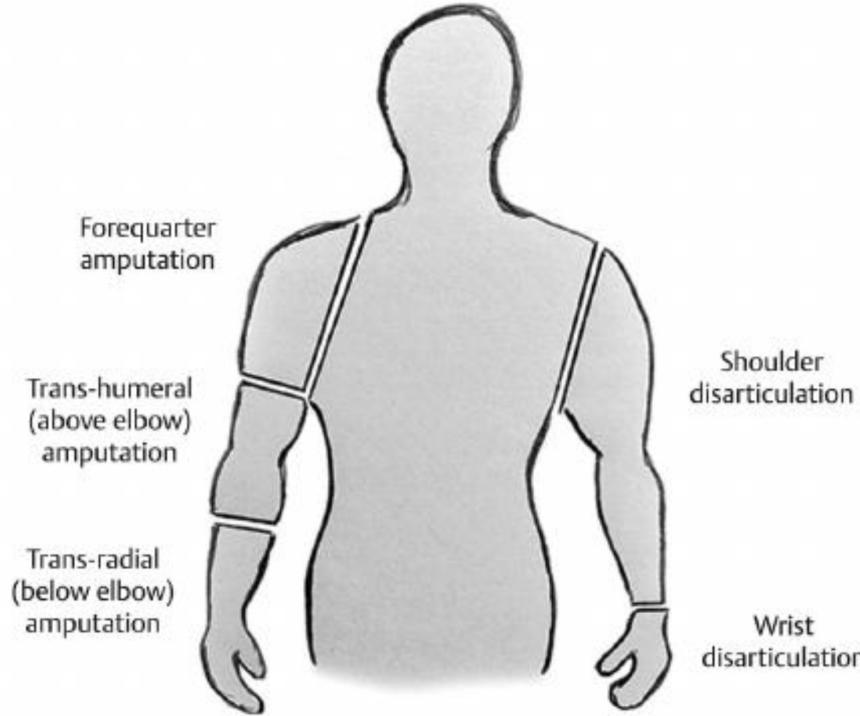
- ❖ Muscles reflects the neural activities



Muscle behaves as “bioscreen” of the neural activity

Ways to interface

❖ Multiple ways to interface muscle



- Invasive
- Non-invasive
- Minimum invasive



Intramuscular



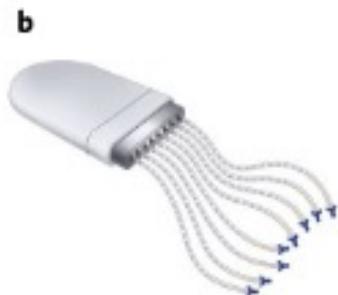
Surface

Invasive Method

❖ Implantable electrode



MyoPlant



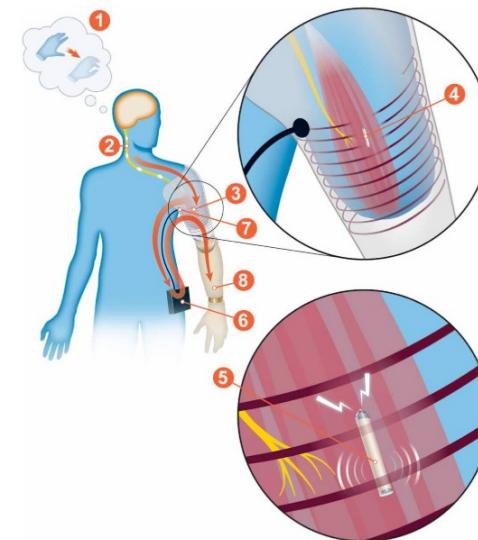
MIRA



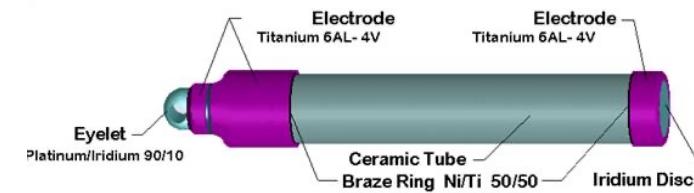
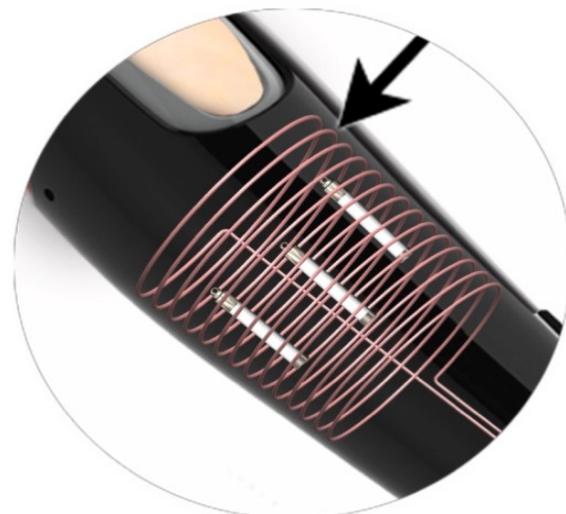
iSens



IMES



Reverse and forward telemetry is used for the signal transmission (transcutaneous magnetic links)



Includes differential amplifier



Non-invasive Method - Materials

❖ Surface EMG



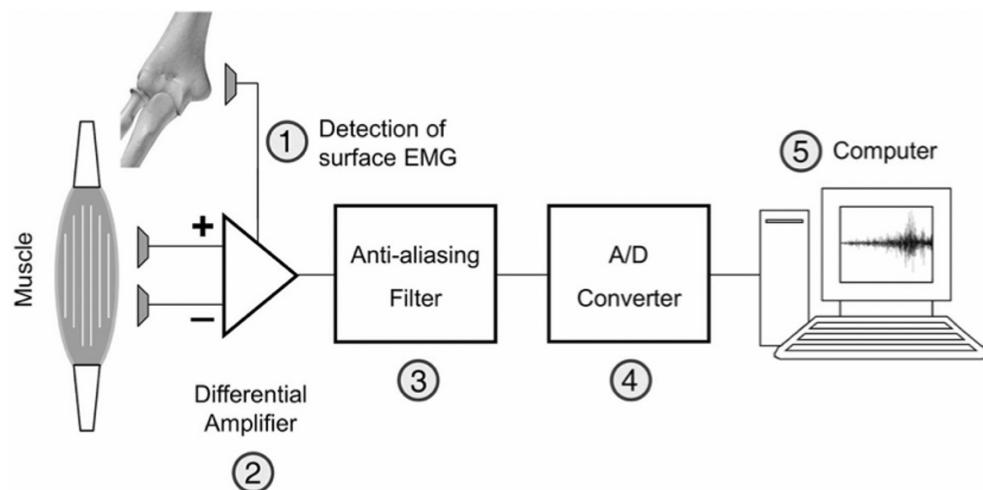
Monopolar



Bipolar



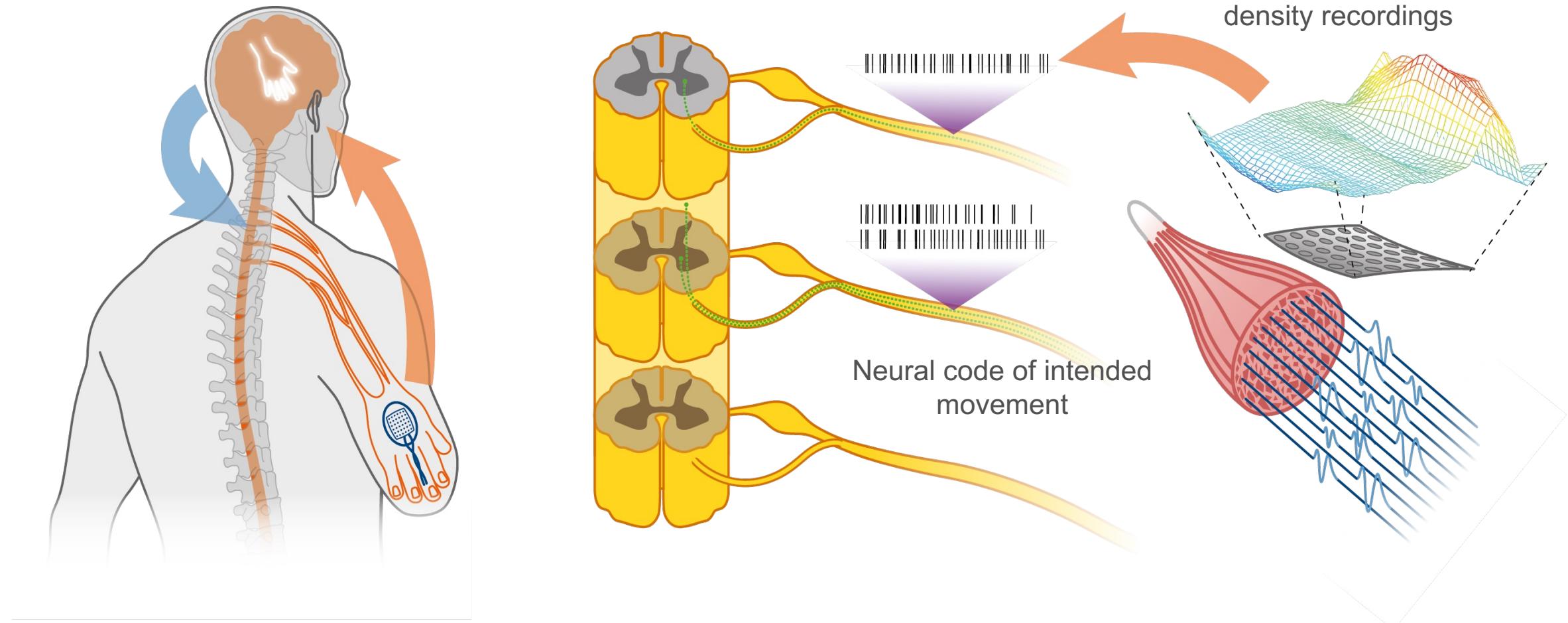
High-density



Amplifier

Non-invasive Method – HD-EMG

- ❖ Spinal signal source separation by HD-EMG

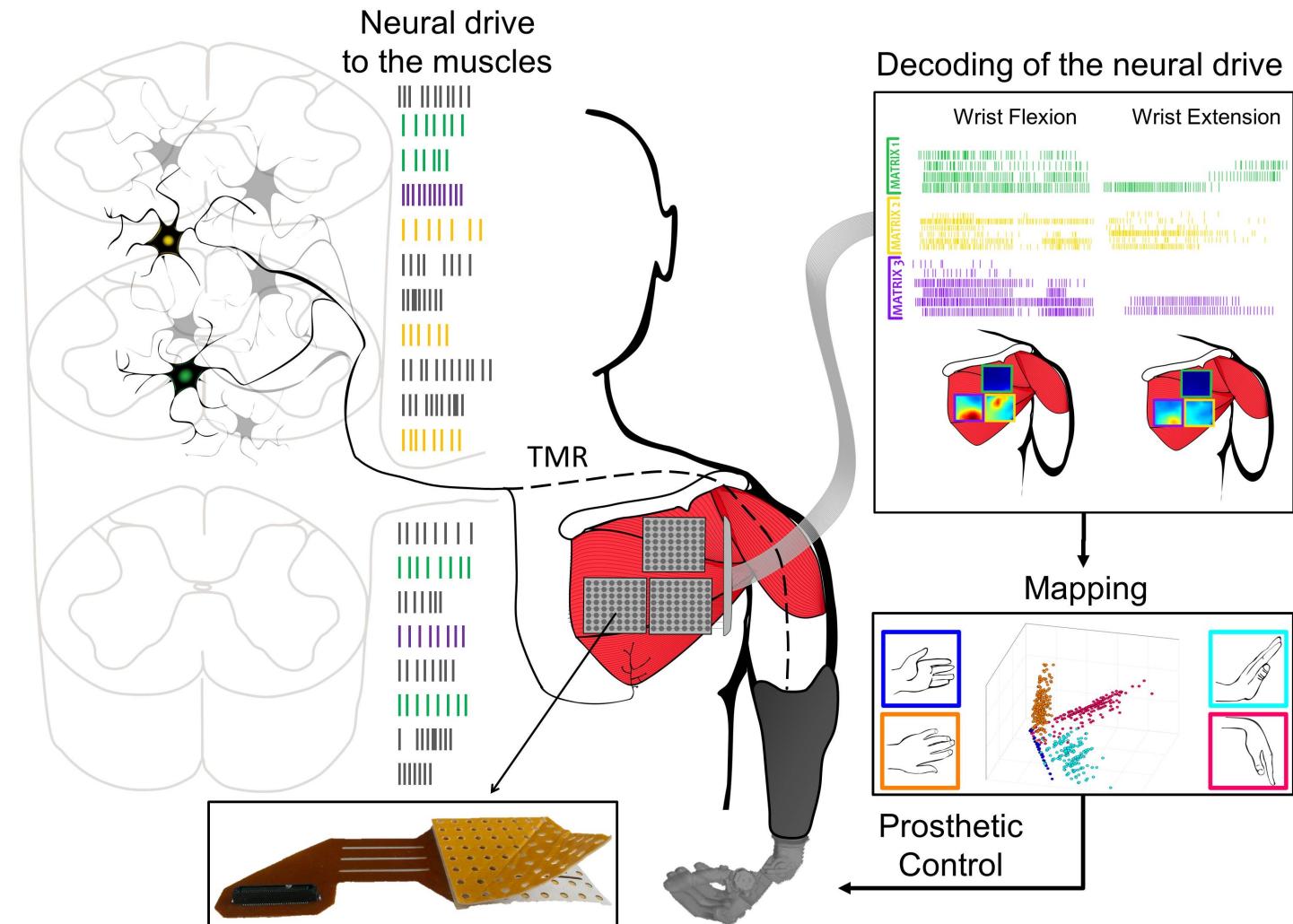
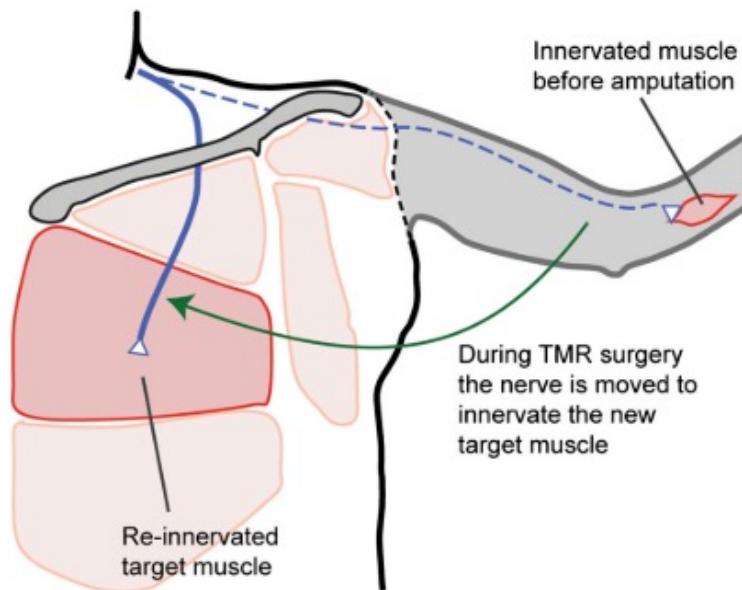


Non-invasive Method - TMR

- ❖ Biological signal source separation by HD-EMG with TMR surgery

Target Muscle Reinnervation

- The reinnervated muscle behaves as a "bioscreen" for the missing limb's neural activity



Roche et al., Current Surgery Reports, 2014

Farina et al., Nature Biomed Eng. 2017

Non-invasive Method - TMR

- ❖ Biological signal source separation by HD-EMG with TMR surgery

ottobock.

UNIVERSITÄTSMEDIZIN
GÖTTINGEN : UMG

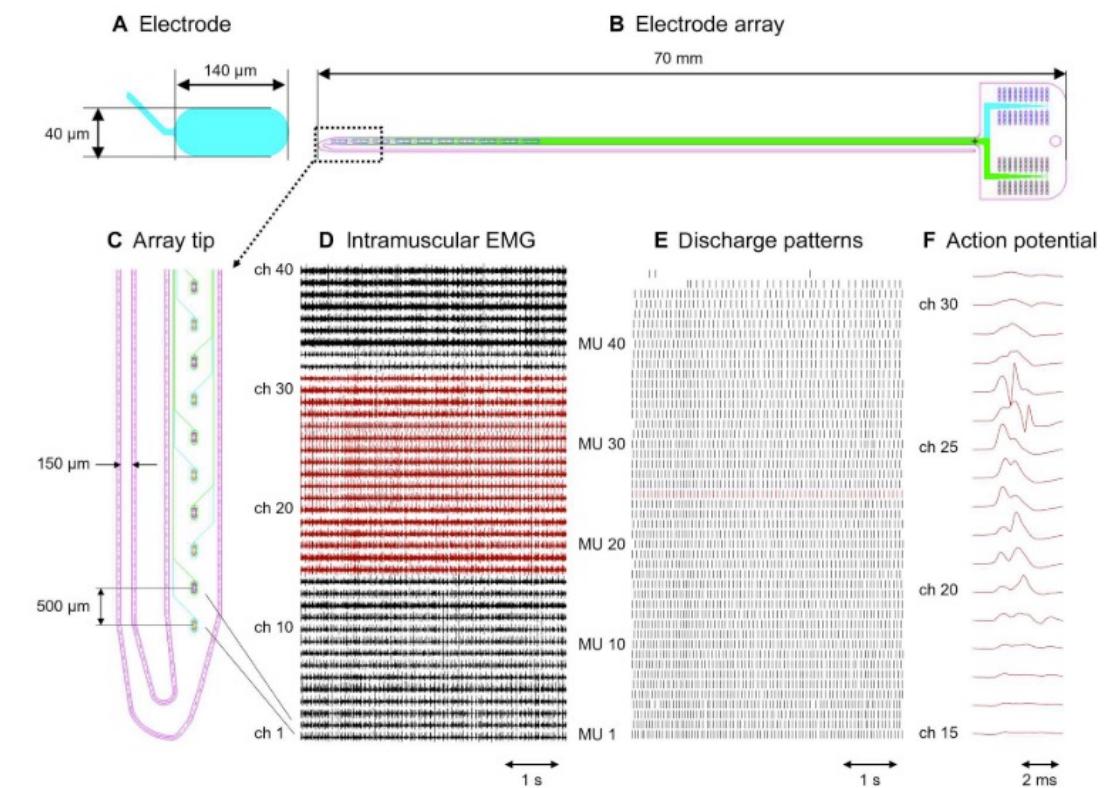
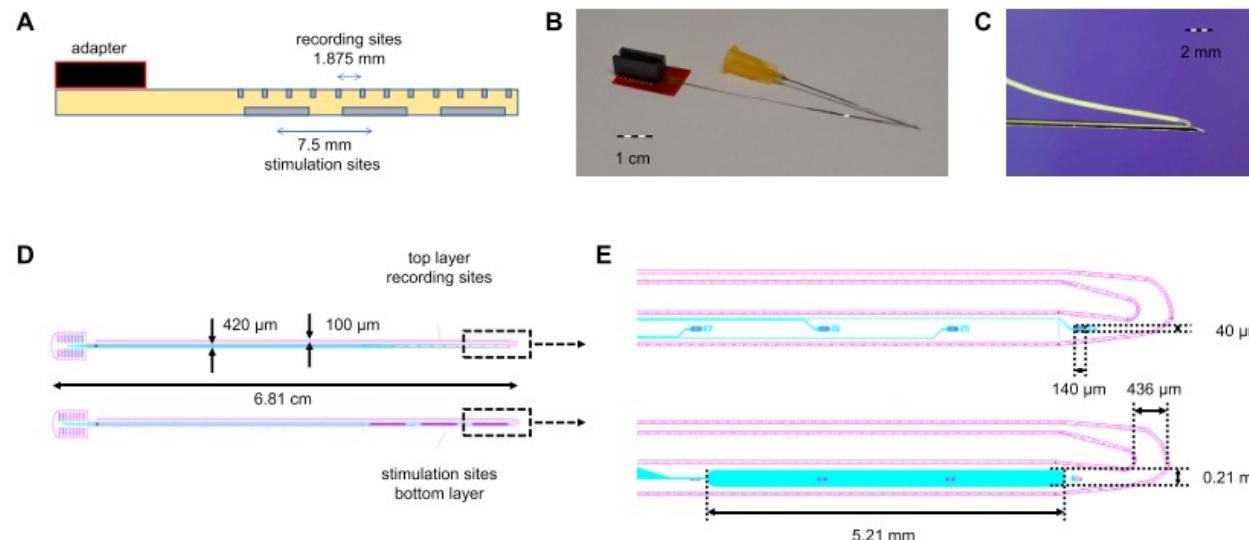
TMR Subject
(9 month post surgery)

Visualisation of the measured potentials

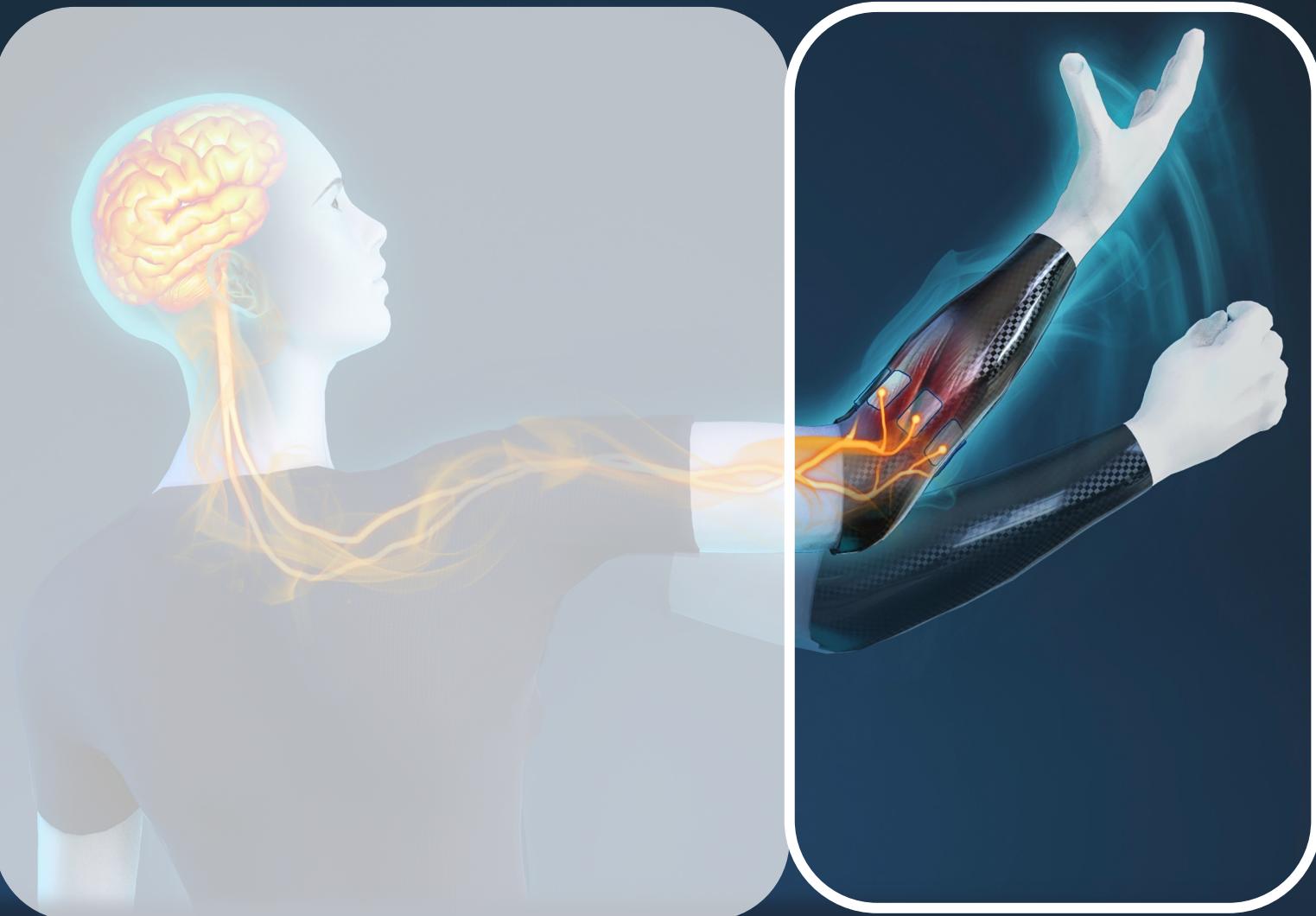
hubertus.rehbaum@bccn.uni-goettingen.de

Minimum Invasive Method

- ❖ Thin-film electrode to overcome sEMG barriers
 - sEMG is difficult to have a connection to the skin
 - sEMG's cross-talk is always the issue



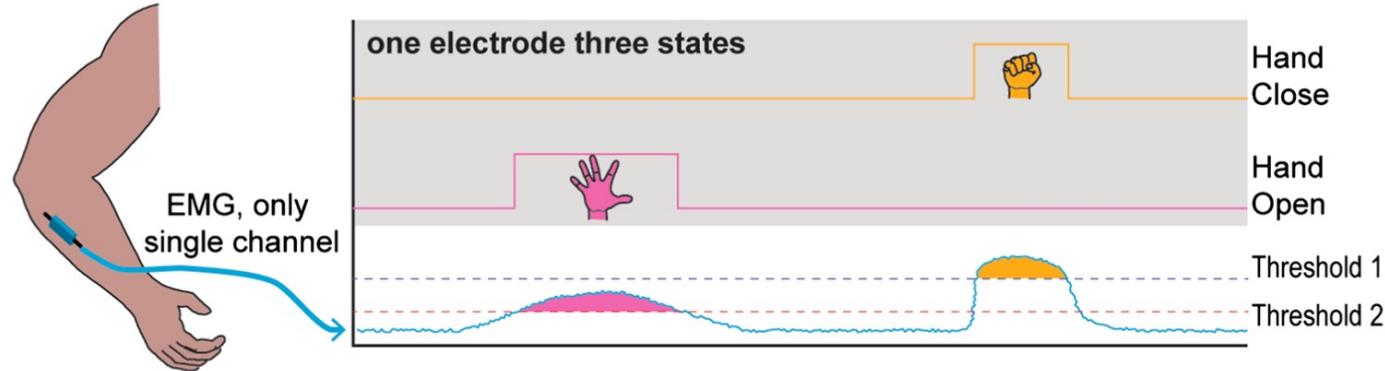
Control strategies



Control strategies – Low-density sEMG (one to two channels)

❖ Early Stage Control Strategies

Single channel threshold based

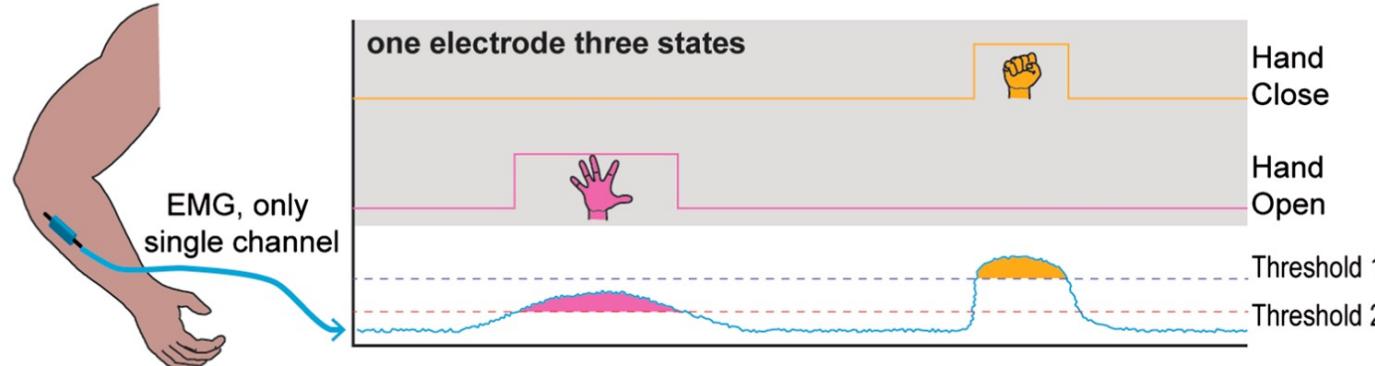


- Using one channel EMG with threshold
- ✓ Easy to implement
- ✓ Robust to the environmental change
- ✗ Number of generated movements is limited

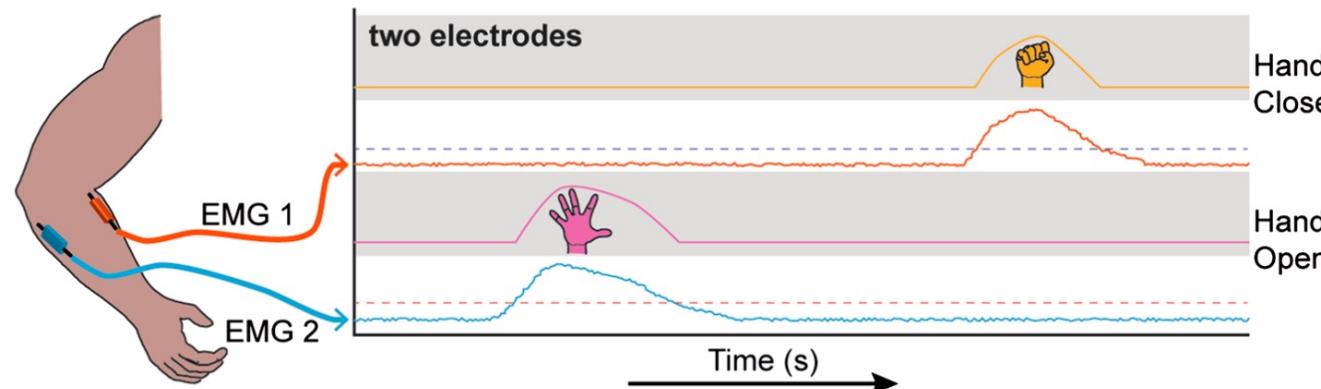
Control strategies – Low-density sEMG (one to two channels)

❖ Early Stage Control Strategies

Single channel threshold based



Two opposing channels



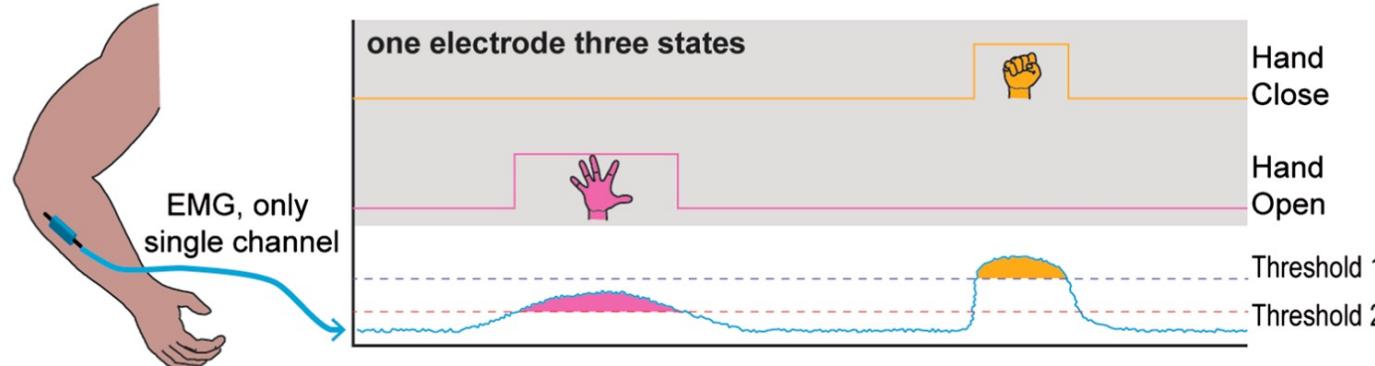
- Using one channel EMG with threshold
- ✓ Easy to implement
- ✓ Robust to the environmental change
- ✗ Number of generated movements is limited

- Controls mechanical output (force, velocity, position, etc)
- Used in commercially available hands (Michelangelo, Hero Arm)
- ✓ Increase in gestures
- ✗ Insufficient for finer movement (e.g., individual finger flexion)
- ✗ Far from multifunctional control

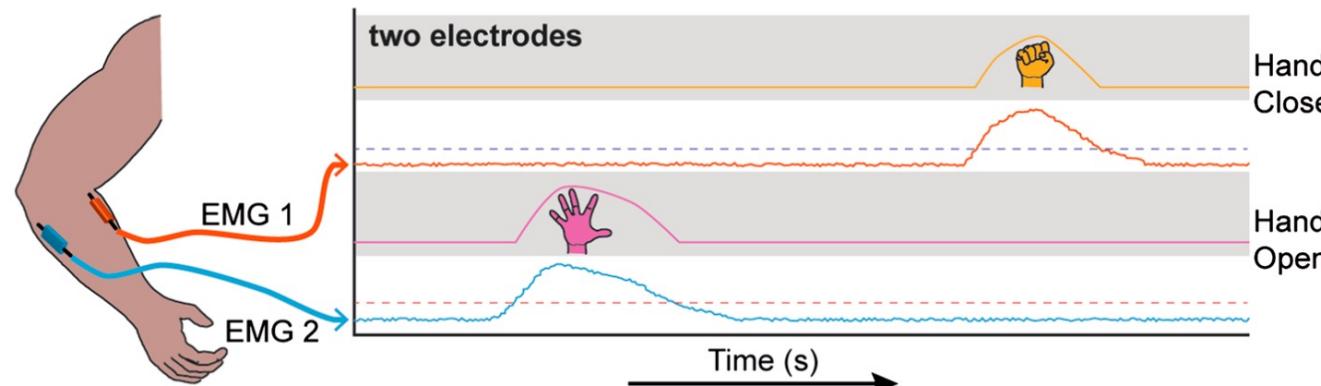
Control strategies – Low-density sEMG (one to two channels)

❖ Early Stage Control Strategies

Single channel threshold based



Two opposing channels



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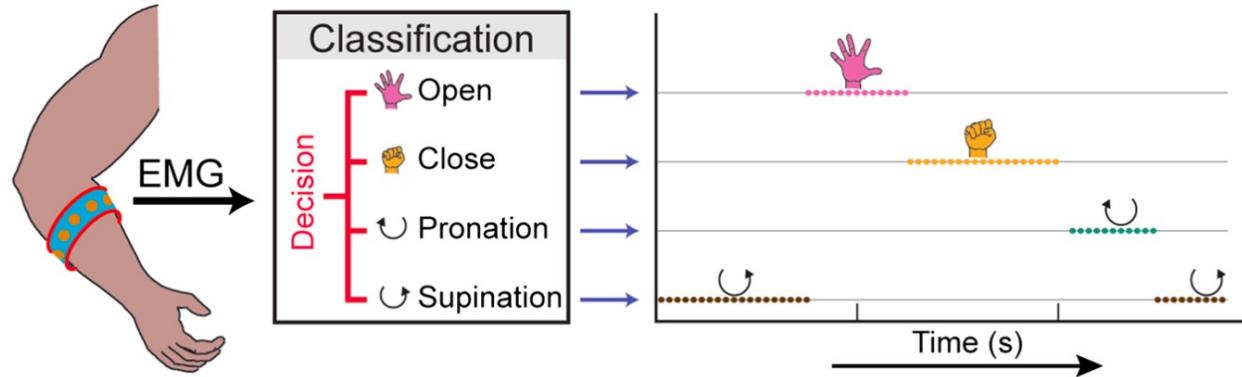
- Controls mechanical output (force, velocity, position, etc)
- Used in commercially available hands (Michelangelo, Hero Arm)
- ✓ Increase in gestures
- ✗ Insufficient for finer movement (e.g., individual finger flexion)
- ✗ Far from multifunctional control

More advanced control strategies have been proposed

Control strategies – Low-density sEMG (8 to 16 channels)

❖ Machine Learning Approach

Pattern Recognition Control

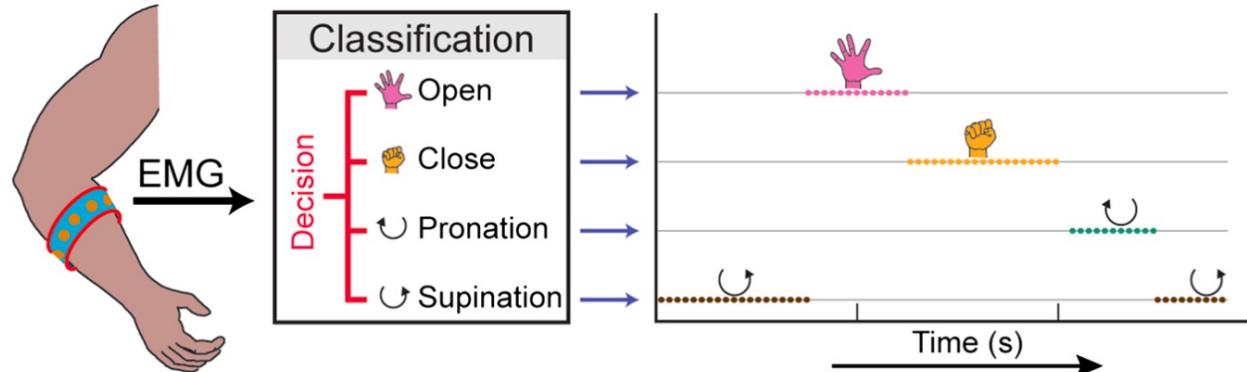


- In sequence, not simultaneously & proportionally (on/off basis)
Methods: Support Vector Machine, K-Nearest Neighbor, Artificial Neural Networks
- ✓ Can achieve multiple gestures
- ✗ Difficult to translate into real-world situations (muscle contraction patterns change, re-calibrate, classification accuracy, etc)

Control strategies – Low-density sEMG (8 to 16 channels)

❖ Machine Learning Approach

Pattern Recognition Control

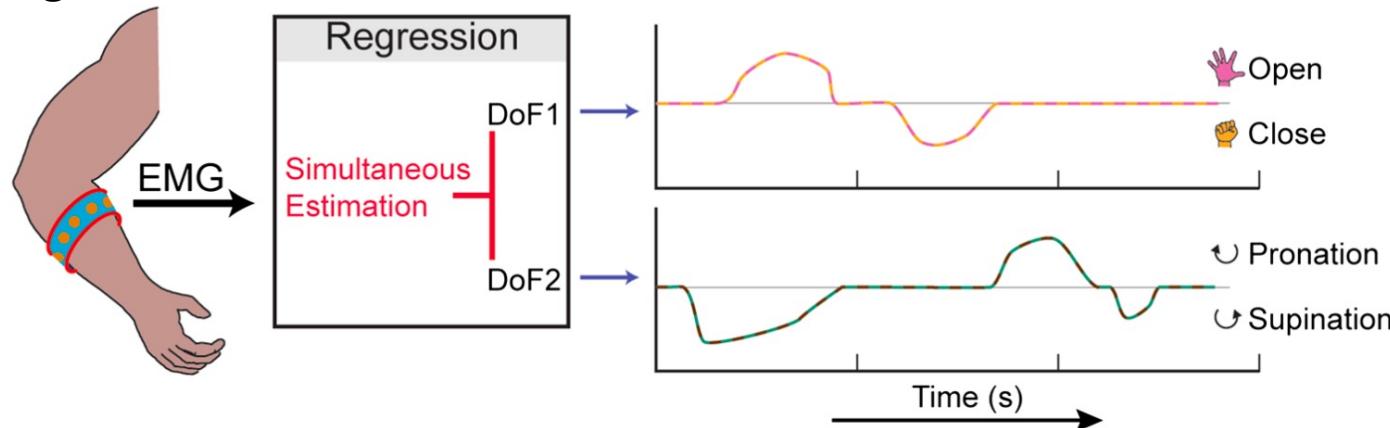


- In sequence, not simultaneously & proportionally (on/off basis)

Methods: Support Vector Machine, K-Nearest Neighbor, Artificial Neural Networks

- ✓ Can achieve multiple gestures
- ✗ Difficult to translate into real-world situations (muscle contraction patterns change, re-calibrate, classification accuracy, etc)

Regression Control



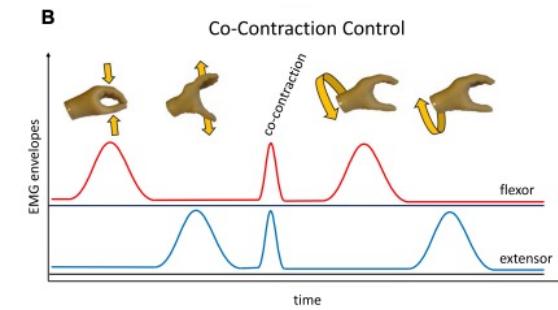
- Simultaneous & proportional control

Methods: Negative Matrix Factorization, Artificial Neural Networks, Linear Regression

- ✓ Intuitive
- ✗ Stable control limited to 2DoF due to cross-talk
- ✗ High separation of the DoF matters
- ✗ Still limited to the lab phase

Control strategies – Low-density sEMG (8 to 16 channels)

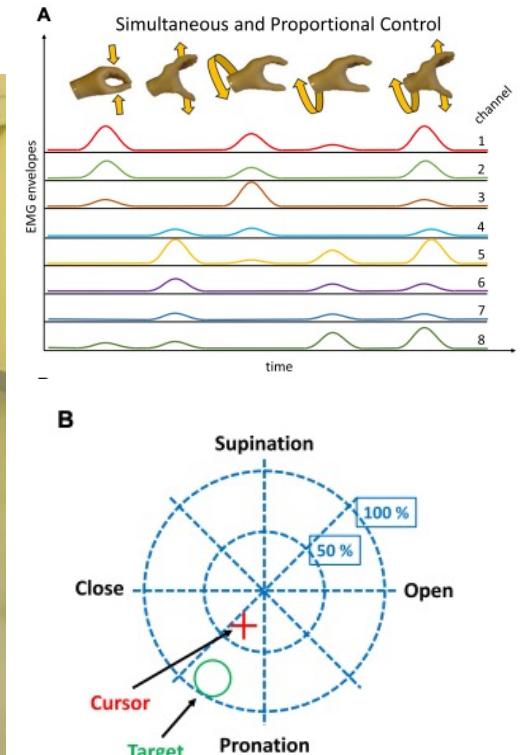
❖ Linear Regressor (2DoF) by 8 EMG Channels



Conventional direct control

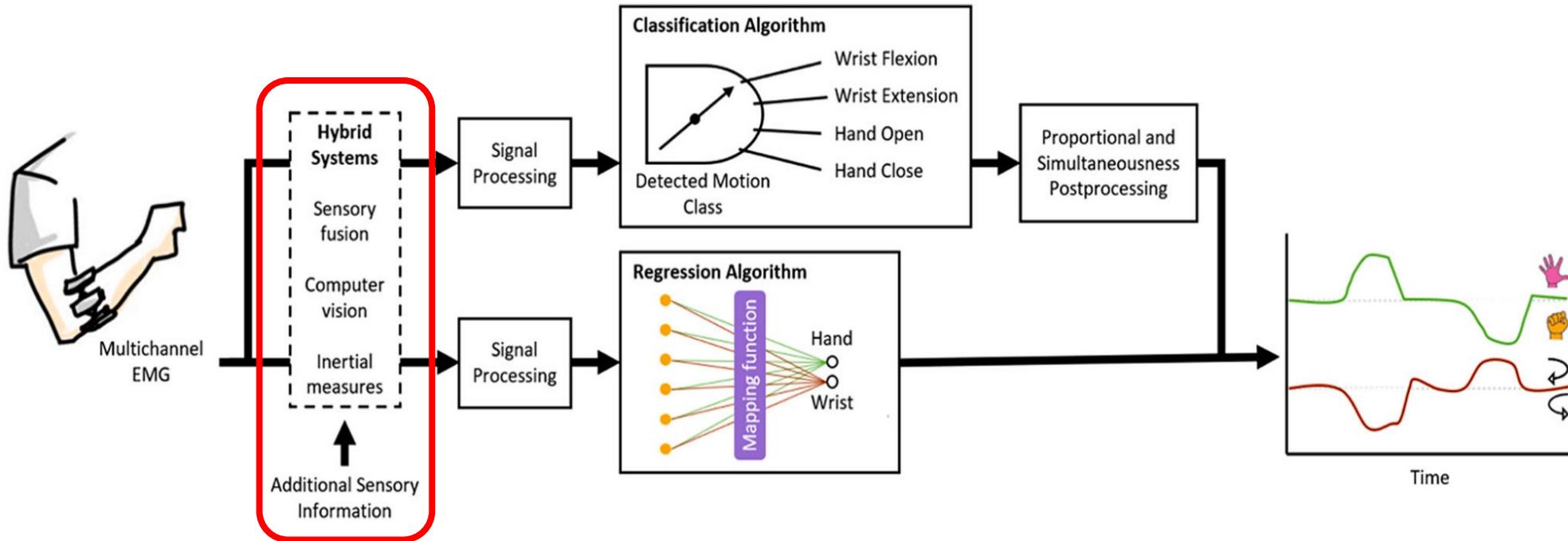
Linear regressor

Intuitive and quicker to complete the task



Control strategies – Low-density sEMG Hybrid Control

❖ Hybrid Systems to Overcome Limitations of Regression Control



➤ Additional information to improve the control accuracy

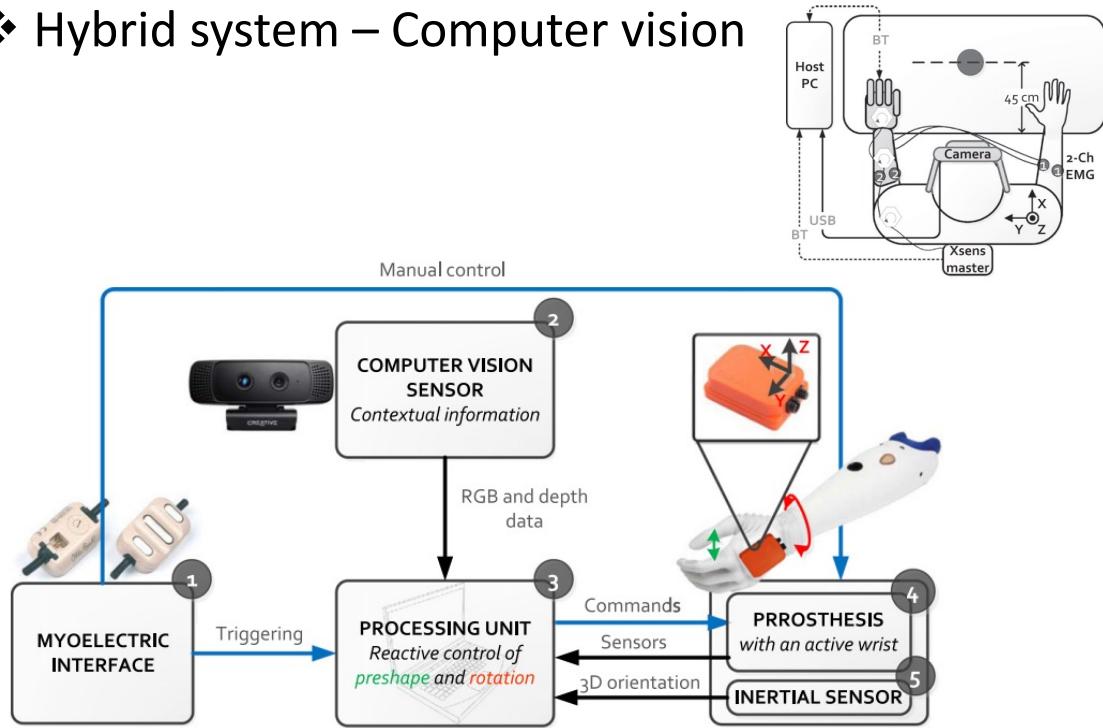
Methods: Multi-modal sensory fusion, Computer vision, etc

✓ Can acquire information (contextual information) that cannot capture by EMG

✗ Still limited in the lab environment

Control strategies – Low-density sEMG Hybrid Control

❖ Hybrid system – Computer vision

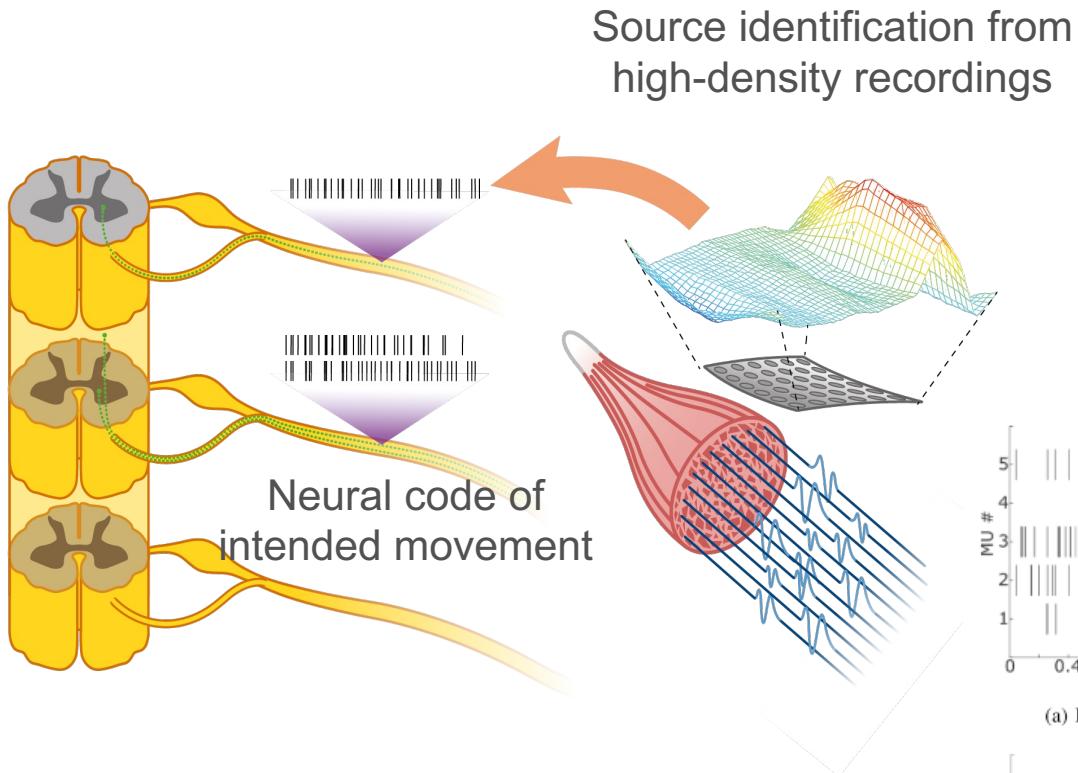


- Simultaneous & proportional control of 3 DoF based on the fusion of computer vision and position/orientation measurements
- Fine-tune the autonomous decisions (semi-automatic control)

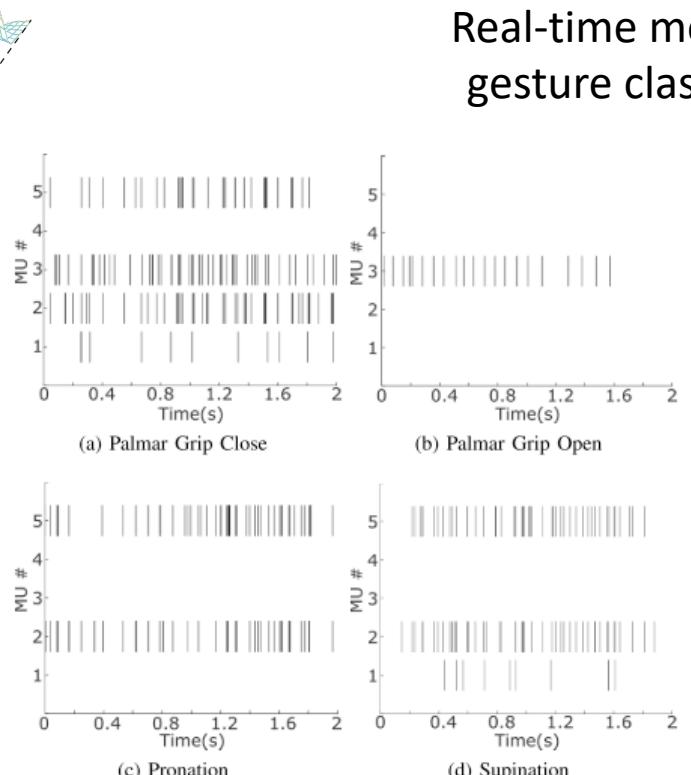
Smoother & higher DoF control than conventional method

Control strategies – High-density sEMG

❖ Motor Unit decomposition



- Motor units activity decomposition by HD-EMG
- Methods: Blind source separation
- ✓ Reliable information about neural activity
- ✗ Increases the computational burden required to the system



Real-time motor unit decomposition
gesture classification (FPGA based)

Output Class	Target Class				Overall Accuracy
	1	2	3	4	
1	143 8.0%	0 0.0%	0 0.0%	0 0.0%	100% 0.0%
2	9 0.5%	297 16.6%	22 1.2%	3 0.2%	89.7% 10.3%
3	12 0.7%	0 0.0%	646 36.2%	34 1.9%	93.4% 6.6%
4	0 0.0%	0 0.0%	65 3.6%	555 31.1%	89.5% 10.5%
	87.2% 12.8%	100% 0.0%	88.1% 11.9%	93.8% 6.3%	91.9% 8.1%

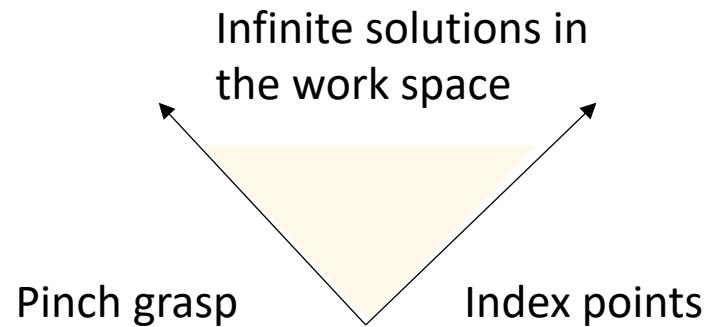
SVM, Class 1: Palmar grip close, Class 2: Palmar grip open, Class 3: Pronation, Class 4: Supination

Control strategies – High-density sEMG

❖ Synergistic approach

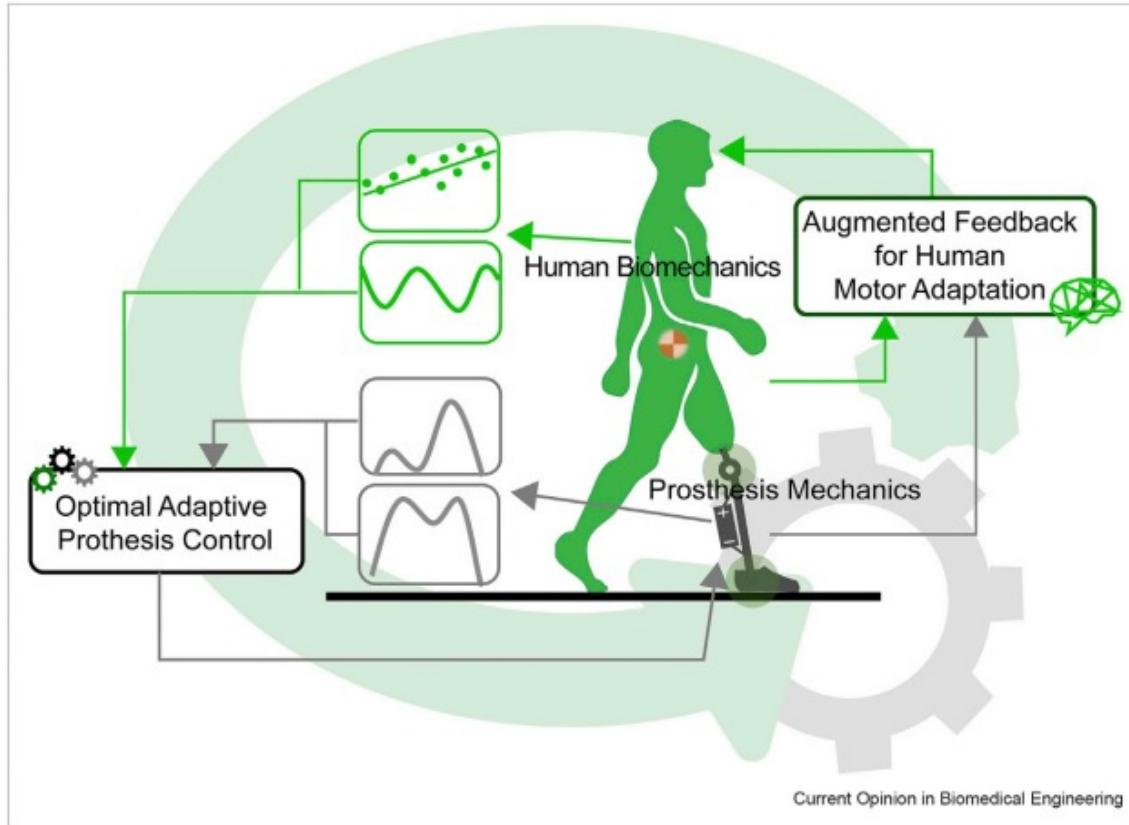
Full integration for true bionic interfacing

Exploring hand capabilities: Index point (y axis).



Control strategies – Adaptive Technique

- ❖ Human-prosthesis symbiosis
- Human motor control and intelligent prosthesis control function as one system



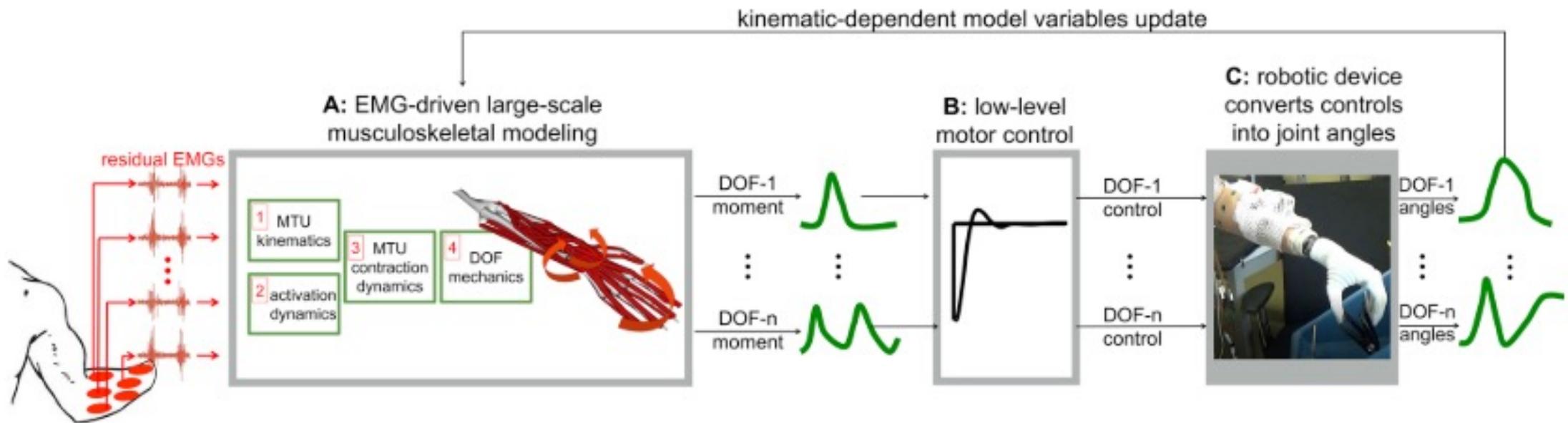
- **Continuous joint coordination**
 - A controller continuously monitors the gait cycle and adjust the joint angles based on the predefined joint coordination
 - ✓ Better adaptability to varied walking speeds and inclination angle
 - ✗ Tuned manually and individually
- **Reinforcement learning**
 - Tune the adaptive parameters in real-time
 - ✓ Model free and prior tuning knowledge free

Control strategies – Model-based approach

- ❖ Biological limbs' joint rotation can be generated by different EMG patterns
- ❖ Vary across individuals, training conditions, arm postures, or tasks



- ❖ Forward musculoskeletal model mimics the biological process
 - Directly incorporates physiological and biomechanical constraints
 - With TMR, this can reconstruct the internal biomechanical representation of missing limbs



Future Direction

- ❖ Next generation clinical prostheses' key areas

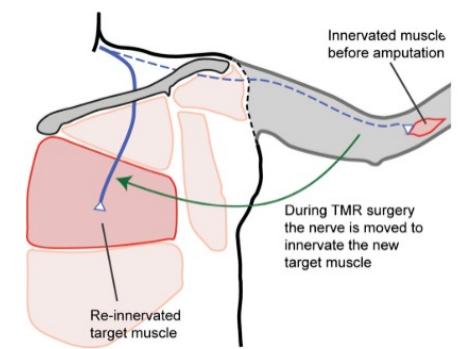


Future Direction

- ❖ Next generation clinical prostheses' key areas

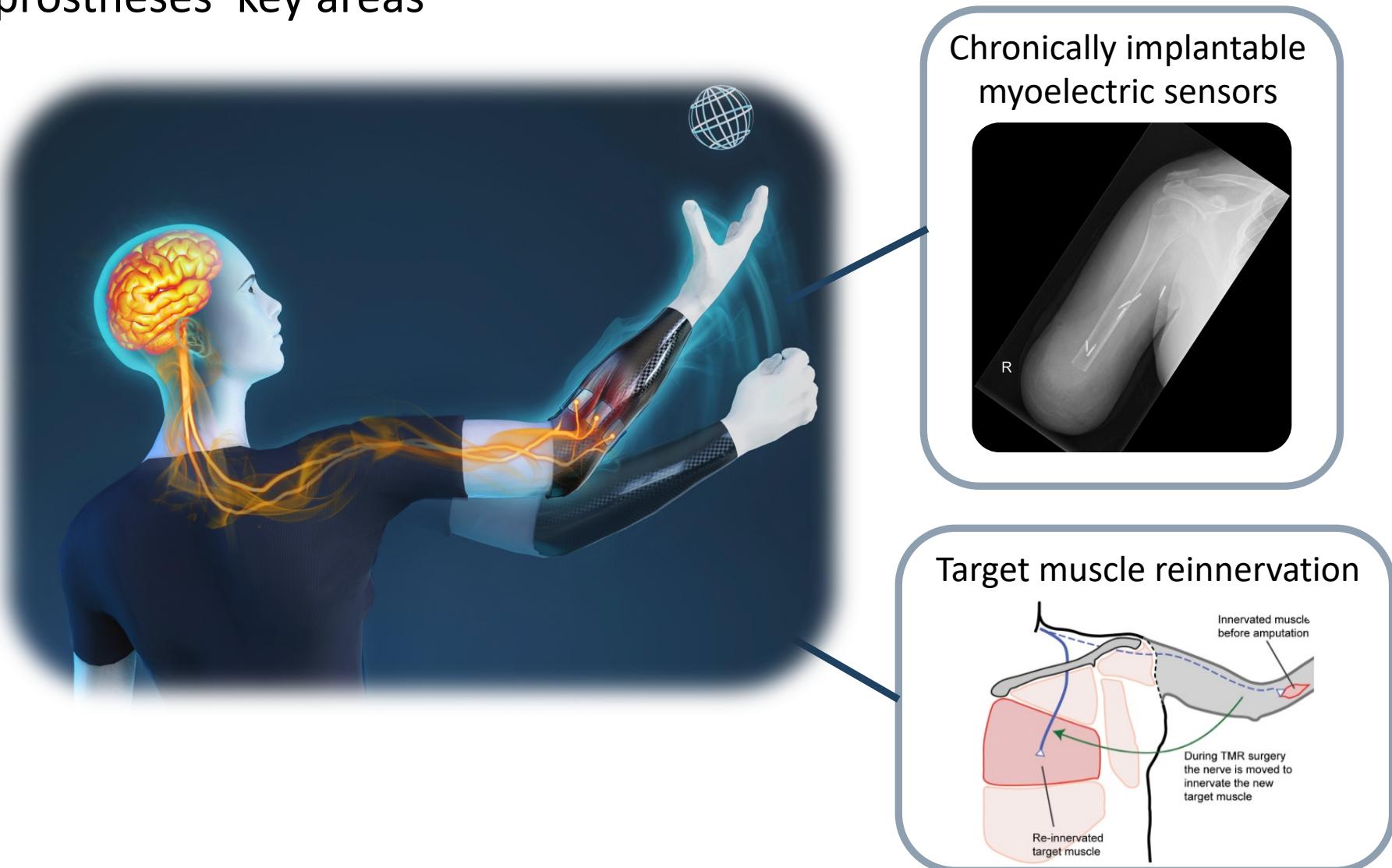


Target muscle reinnervation



Future Direction

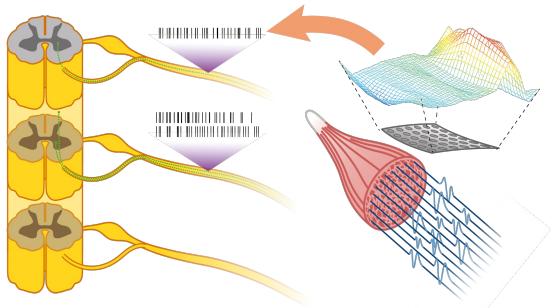
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Future Direction

❖ Next generation clinical prostheses' key areas

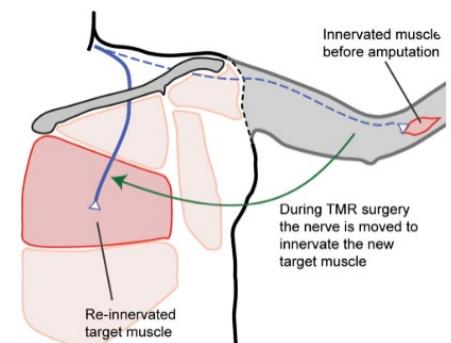
Advanced control algorithms



Chronically implantable myoelectric sensors



Target muscle reinnervation



Hands on!

- Offline algorithm development-

Mini Project System Overview



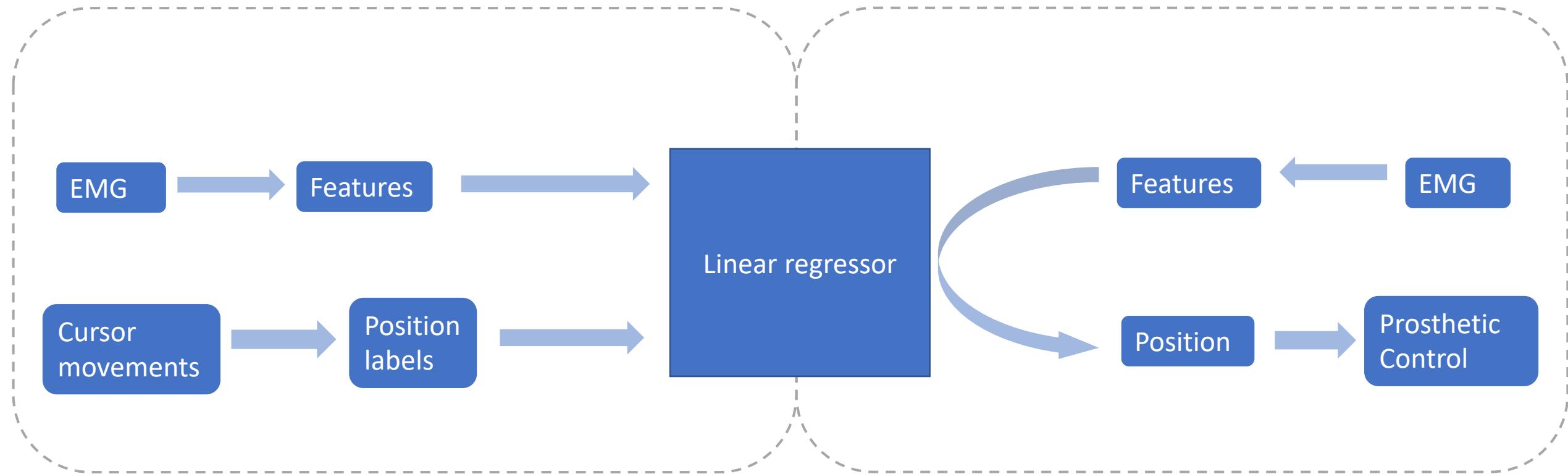
1st Part: Demonstration real time system

Demonstrate with MyoControl.m by organiser:

1. App = MyoControl
2. Data collection
3. Training regressor
4. Real time control cursor on virtual cursor

Offline analysis:
Feature extraction and linear regression

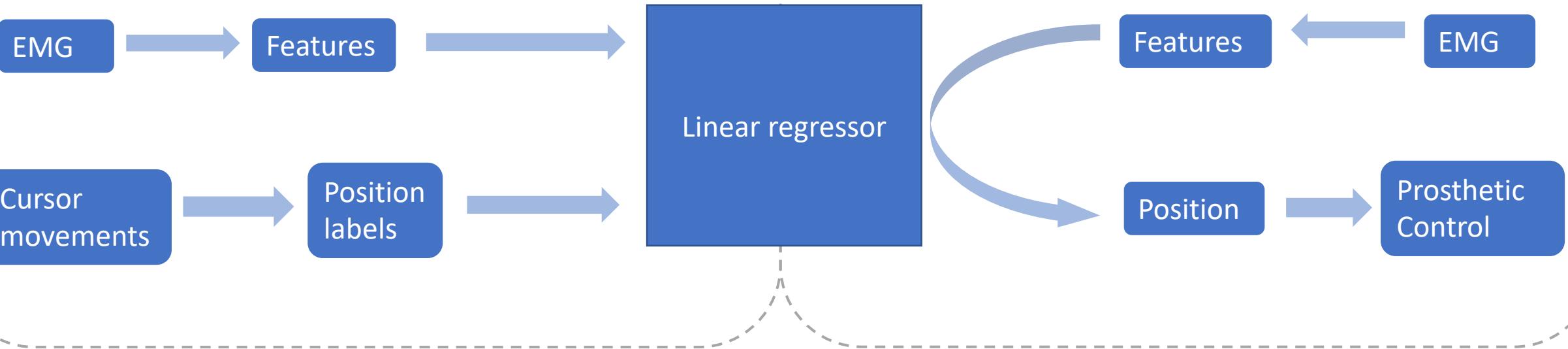
Training the algorithm



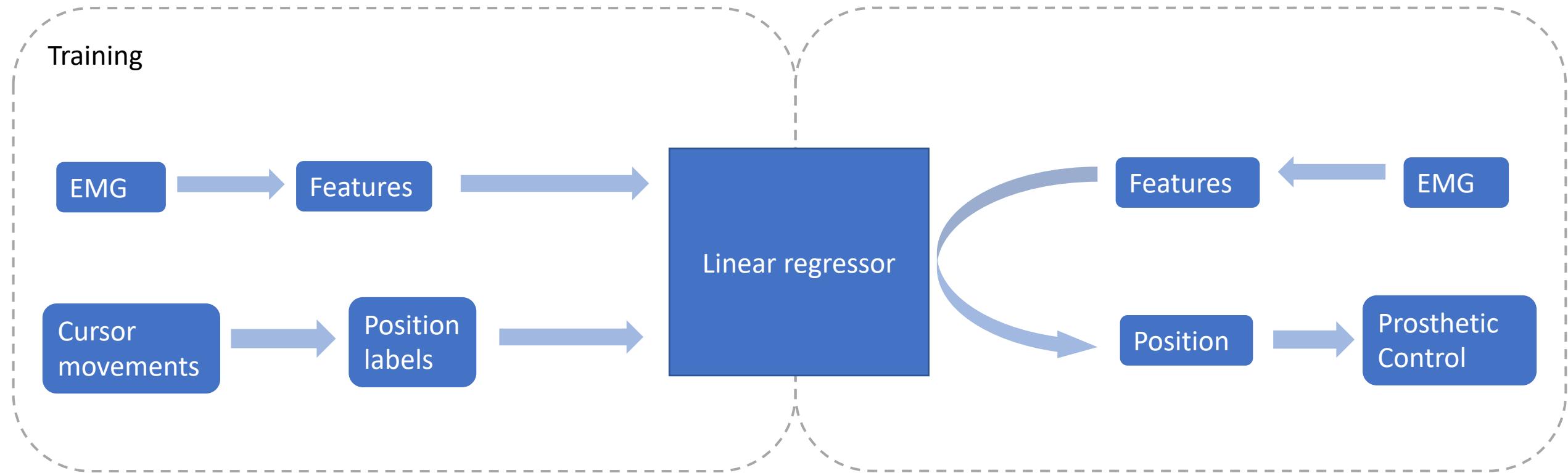
Training the algorithm



What is this part called?



Training the algorithm



Training the algorithm

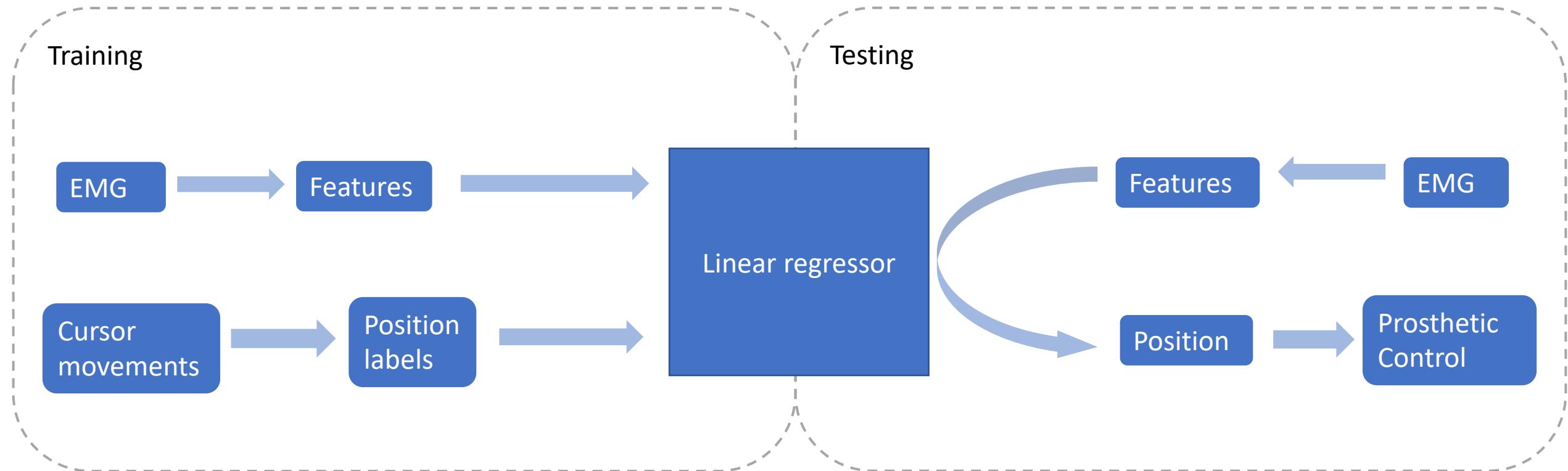


Training

What is this part called?



Training the algorithm



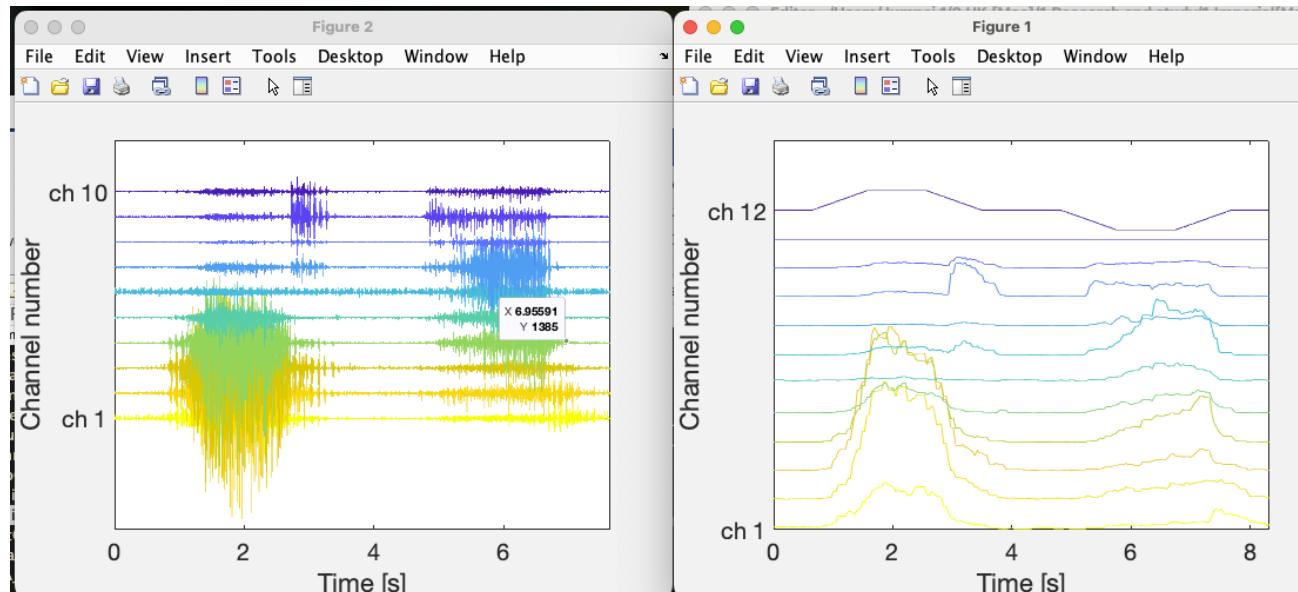
1. Plot Trial

Visualise the sEMG signals

- Check the the sEMG signals on pre-recorded data – rawEMG and rms
- “Demo data” -> “TrainingData” -> any data you want

```
15 %% 1. Plot trial
16 %close all;
17 % Get the file
18 [infile,path] = uigetfile();
19 file      = load(fullfile(path,nfile));
20
21 % Input data to test with the regressor
22 RecInfo    = file.RecInfo;      % Rms data to test
23
24 figure(1)
25 nchan      = size(RecInfo.EMGRMS,2);          % define the number of channels
26 % Plotting function
27 % plotCh(data, number of channels, Sampling frequency)
28 dataToPlot = [RecInfo.EMGRMS';RecInfo.Labels'];
29 plotCh(dataToPlot.*10, nchan+2, 25)           % to include in the plot the labels
30                                         % Plot data and labels, 25 Hz frequency
31
32 % Plot of the rms Data
33 figure(2)
34 plotCh(RecInfo.EMGraw', nchan, 1000)
35 % Plot raw data
```

Result



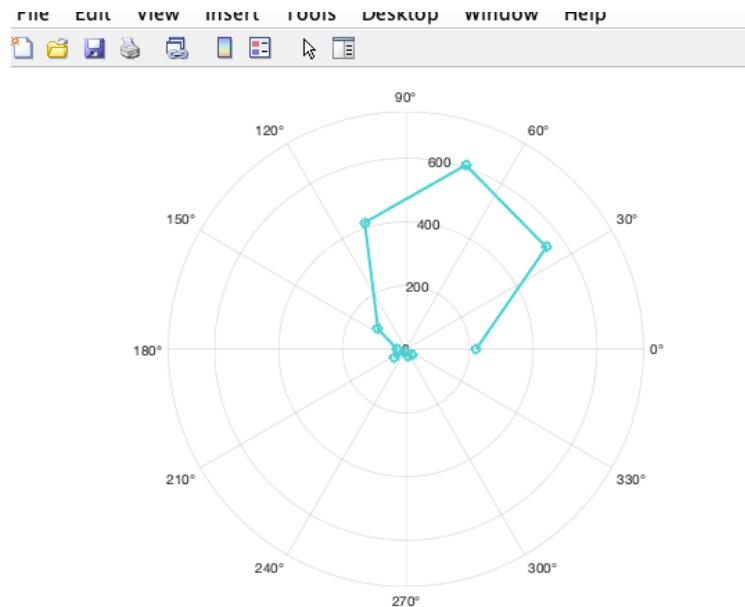
2. Plot over time

Visualise the sEMG signals

- Plotting the EMG RMS value in a polar plot

```
34
35 %% 2. Plot over time
36 %close all;
37
38 FP      = figure(3);
39 FP.Color = [1,1,1];
40 rlim    = max(max(RecInfo.EMGRMS));
41 %theta   = deg2rad([(36):36:(360)]);
42 theta   = deg2rad([0:360/nchan:360]);
43 for sample = 1 : length(RecInfo.EMGRMS)
44
45 FP = polarplot(theta(1:end-1),RecInfo.EMGRMS(sample,1:nchan),'o-','linewidth',2,'color',[0, 0.8, 0.8]);
46 %FP = polarplot(theta,RecInfo.EMGRMS(sample,[2:10,1]),'o-','linewidth',2,'color',[0, 0.8, 0.8]);
47
48 hold off
49 FP.Parent.RLim = [0,rlim];
50
51 pause(0.04)
52 drawnow;
53
54 end
```

Result



3.A - Concatenate all data

Concatenate the existing data

- “DemoData” -> “TrainingData”-> open

```

55 % 3.A - Concatenate all data
56
57 % Concatenate data
58 path = uigetdir();
59 % Scan all the recording files in the folder
60 ToScan = fullfile(path, '*rec*.mat');
61 files = dir(ToScan);
62
63 % Arrays to concatenate the data
64 rawEMG = []; % Array for the raw EMG
65 feats_aux = []; % Array for the rms EMG
66 labels_aux = []; % Array for the training labels
67
68 for nfile = 1: length(files)
69     % Load the file - training data
70     FileToLoad = fullfile(path,files(nfile).name);
71     load(FileToLoad);
72
73     fprintf(strcat('Loading file : ', files(nfile).name, '\n'));
74
75     % Joint data
76     feats_aux = [feats_aux; RecInfo.EMGRMS];
77     labels_aux = [labels_aux; RecInfo.Labels];
78     rawEMG = [rawEMG; RecInfo.EMGraw];
79 end

```

```

81 %% 3.B - Plotting of the training data and labels
82
83 % Plot of the Raw Data
84 figure(2)
85 plotCh(rawEMG', nchan, 1000)
86
87 % Plot of the raw Data and labels
88 figure(3);
89 nchan = size(feats_aux,2);
90 plotCh([feats_aux';labels_aux'].*10, nchan+2, 25)
91

```

3.B - Plotting of the training data and labels

3.C - Implement RMS feature extraction given a raw EMG window – [T1A_ExtractRms.m]

Task 1: Create RMS function – 10min

```

% DataRmsEMG = T1A_ExtractRMS(DataInRawEMG)

dOut(samplect,:) = T1A_ExtractRms(DataI);
Evaluate Selection in Command Window F7
% TO COMPLETE BY THE STUDENT
Open "T1A_ExtractRms" F6
Help on "T1A_ExtractRms" F1
samplect = samplect + 1;

end

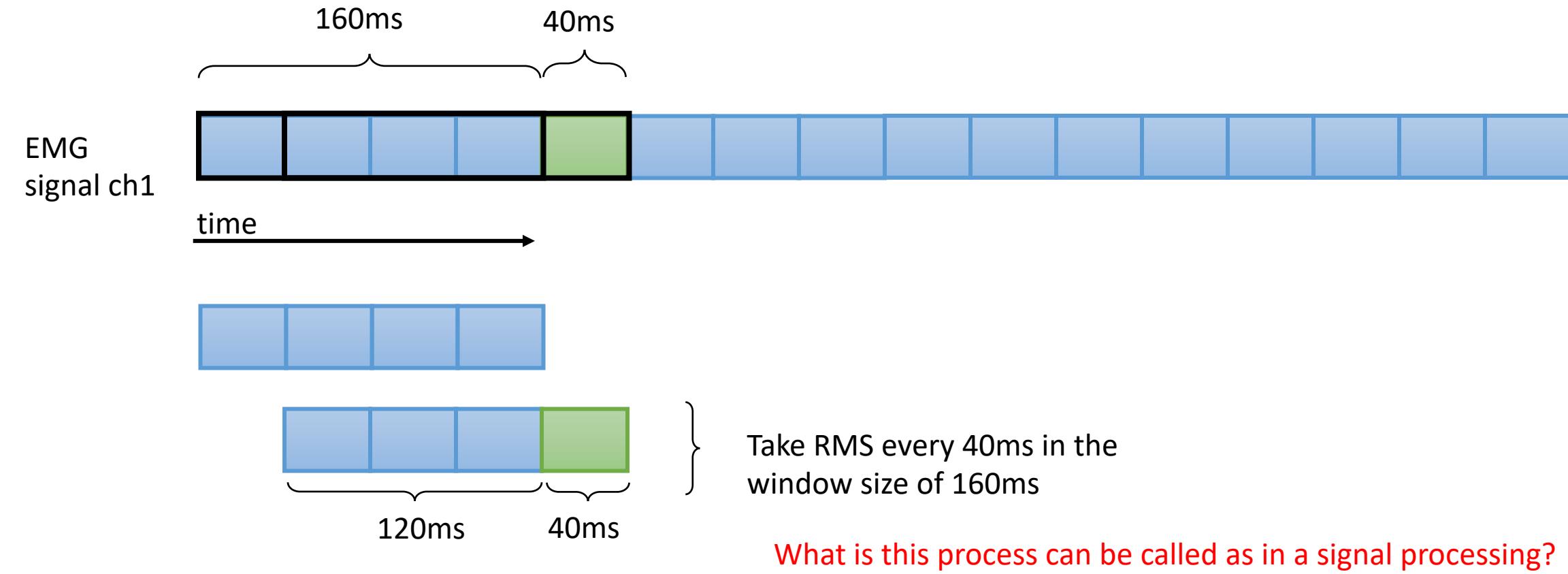
```

```

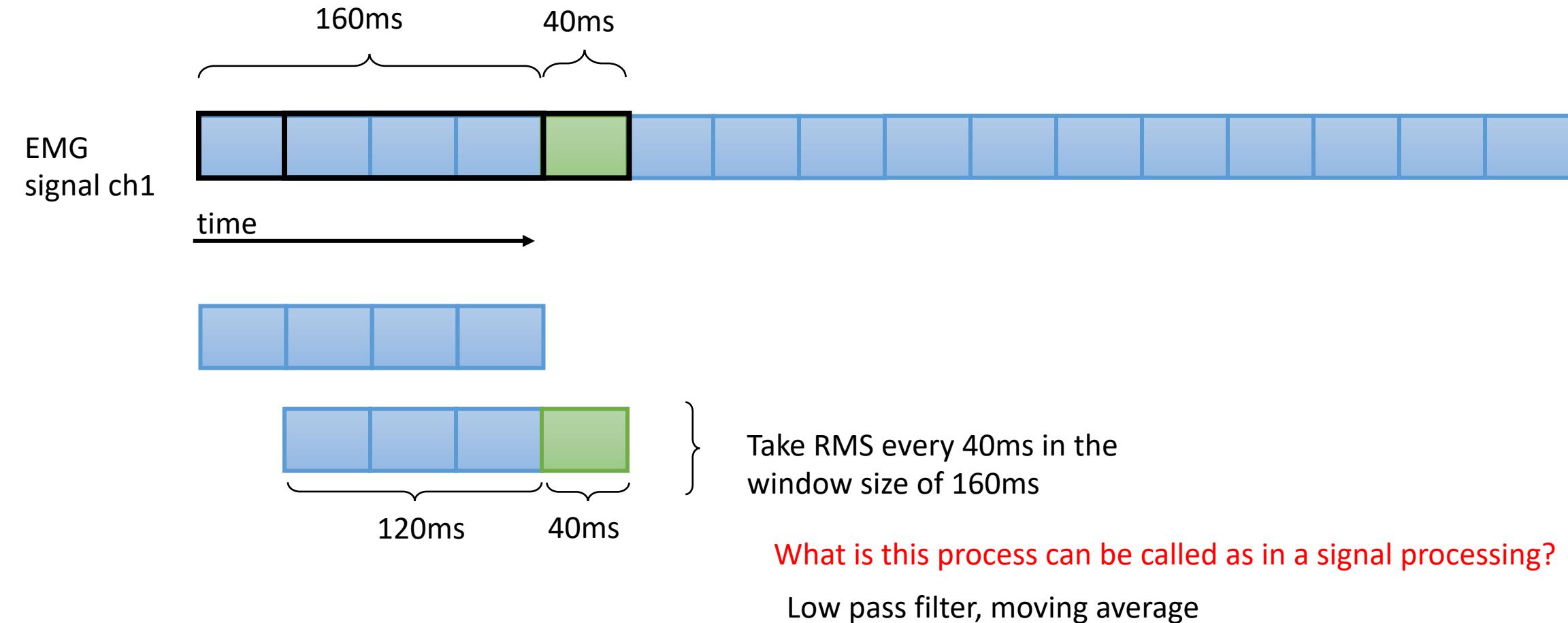
92 %% 3.C - Extract features: RMS
93 Rmswindow = 160;
94 BufSize = 40;
95 samplect = 1;
96 nchan = size(feats_aux,2);
97
98 % RMS data output
99 dOut = zeros(round(length(rawEMG)/BufSize) , nchan);
100
101 for n = 1:round(length(rawEMG)/BufSize)-(Rmswindow/BufSize)
102
103     if n == 1
104         DataI = rawEMG(1:Rmswindow,:);
105     else
106         DataI = rawEMG((BufSize * (n-1) + 1):(BufSize * (n-1) + Rmswindow,:));
107     end
108
109 % FUNCTION TO IMPLEMENT BY THE STUDENT
110 % DataRmsEMG = T1A_ExtractRMS(DataInRawEMG)
111
112 dOut(samplect,:) = T1A_ExtractRms(DataI);
113
114 % TO COMPLETE BY THE STUDENT
115 samplect = samplect + 1;
116
117
118
119 plotCh(dOut.*10, nchan, 25) % Plot data and labels, 25 Hz frequency
120
121
122

```

Windowing for feature extraction



Windowing for feature extraction



RMS



How does the RMS formula look like?

- x_i : EMG value
- n : number of samples
- In this case n is the window size (160ms)
- We calculate the RMS for each channel
- => 1 feature for each channel at each windowed timepoint

RMS



How does the RMS formula look like?

$$RMS = \sqrt{\frac{1}{n} \sum_i x_i^2}$$

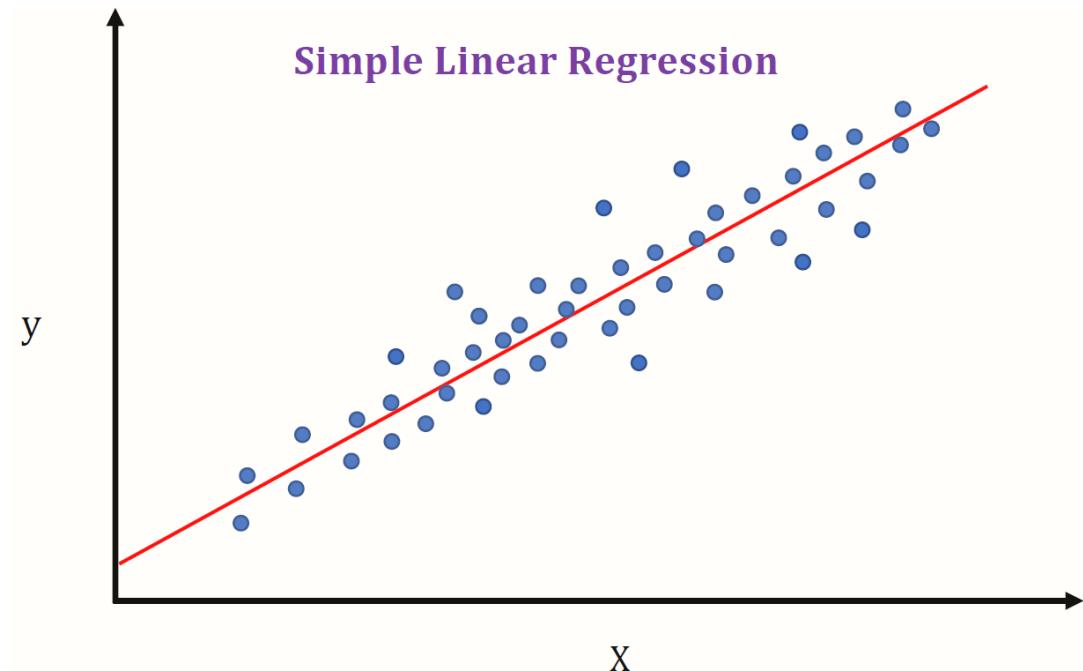
- x_i : EMG value
- n : number of samples
- In this case n is the window size (160ms)
- We calculate the RMS for each channel
- => 1 feature for each channel at each windowed timepoint

Linear Regression



How does the linear regression formula look like?

- y : Movement
- X : EMG feature
- m : slope / regression coefficient
- b : intercept



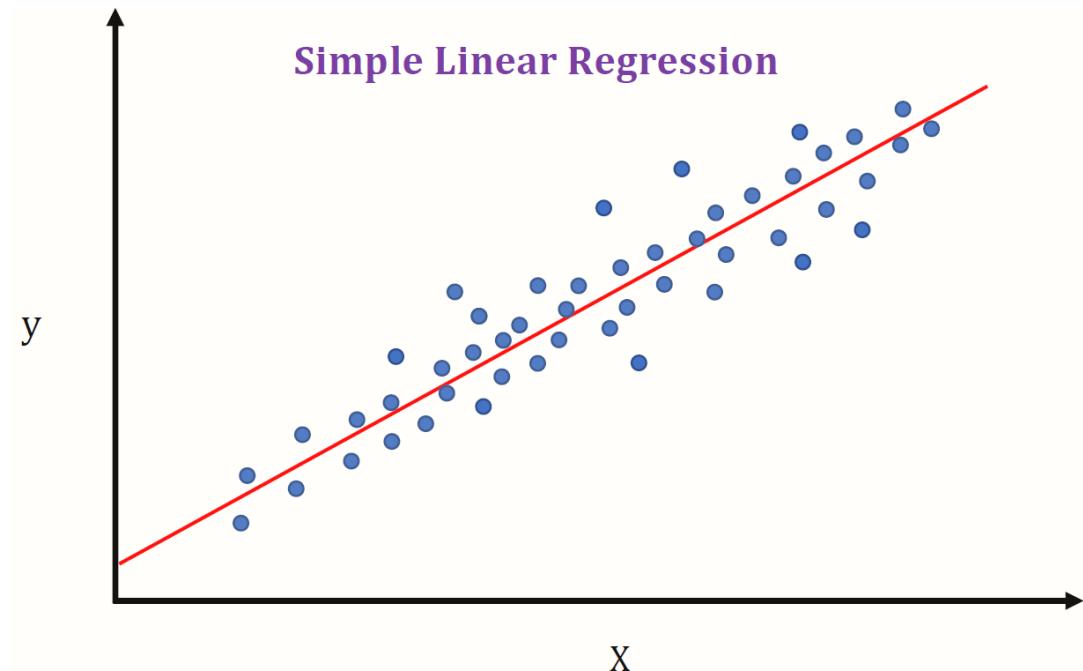
- Simple Linear regression – one angle at a time
- We will calculate the coefficients for each angle
- Functions in Matlab that help you extract the regression coefficients

Linear Regression



How does the linear regression formula look like?

- $y = mX + b$
- y : Movement
- X : EMG feature
- m : slope / regression coefficient
- b : intercept



- Simple Linear regression – one angle at a time
- We will calculate the coefficients for each angle
- Functions in Matlab that help you extract the regression coefficients

3.D – Train regressor

Implement linear regression given pre-recorded data and labels – [T1B_TrainReg.m]

Task 2: Create linear regressor function – 20min

```
123 %% 3.D – Train regressor --- To complete by the student
124 labels = labels_aux; % [DOFs x length recording] – [2 x Length recording]
125 feats = feats_aux; % [channels x length recording]
126
127 % FUNCTION TO IMPLEMENT BY THE STUDENT -----
128 RegCoef = T1B_TrainReg(feats, labels);
129
130 %-----
```

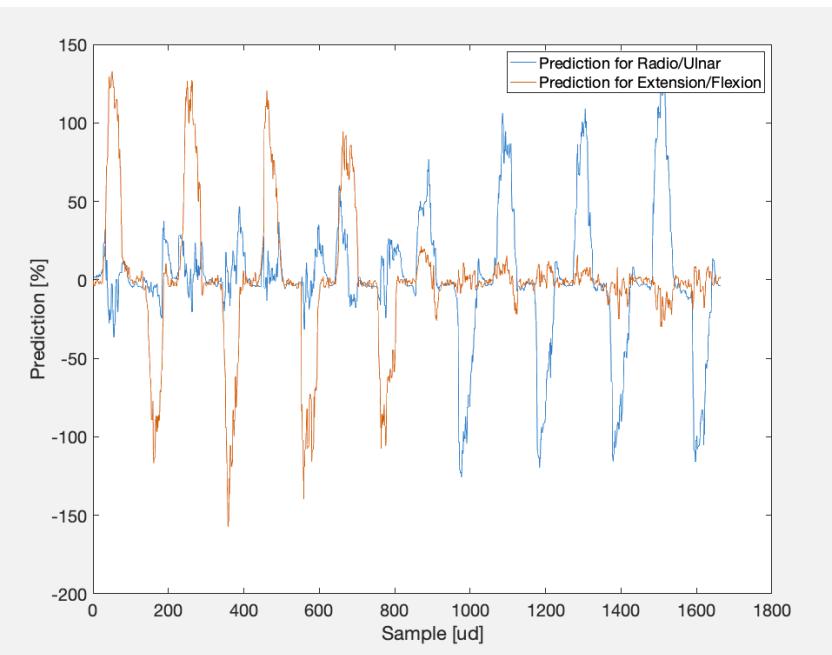
3.E – Test the regressor output

- Implement testing of the linear regression – [T1C_TestReg.m]

Task 3: Create the testing linear regressor function – 10min

```
130 %% 3.E Test the regressor output
131
132 lengthRecording = length(feats);
133
134 % test the data by each sample
135 for sample = 1:lengthRecording
136     trEst(sample,:) = T1C_TestReg([1,feats(sample,:)], RegCoef);
137 end
138
139 % Plot the prediction of the 2 DOF
140 % Positive side represents Radio/Extension prediciton
141 % Negative side represents Ulnar/Flexion
142 plot(trEst)
143 legend('Prediction for Radio/Ulnar','Prediction for Extension/Flexion');
144 set(gca,'FontSize',20);
145 xlabel('Sample [ud]');
146 ylabel('Prediction [%]');
147 %% 3.F – Save the regressor
148 save(fullfile(path,'CoefReg.mat'), 'RegCoef');
149
150 fprintf('Regressor completely saved! \n')
```

Result



- Flex/Ext and Radio/Ulnar movement
- Cross talk between two types of movements
 - The limitation of sEMG

```
147 %% 3.F – Save the regressor
148 save(fullfile(path,'CoefReg.mat'), 'RegCoef');
149
150 fprintf('Regressor completely saved! \n')
```

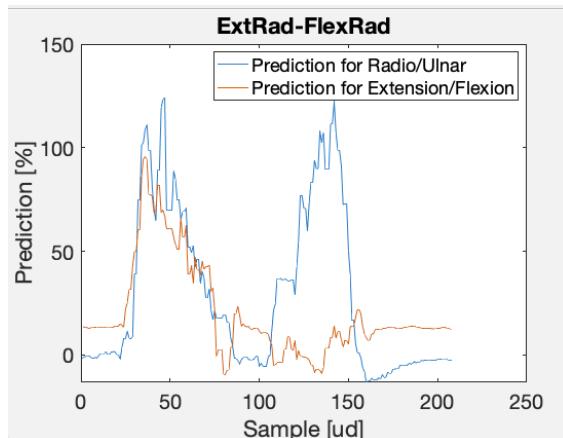
3.F – Save the regressor

3.G – Test the regressor with new Data

- “DemoData” -> “TestData” -> any data you want to see
- Plot prediction with the pre-recorded training data
- Plot prediction with the pre-recorded testing data
- Save regressor coefficients

```
151 %% 3.G – Test the regressor with new Data
152 % Get the file
153 [infile,path] = uigetfile();
154 file = load(fullfile(path,infile));
155
156 % Input data to test with the regressor
157 inputData = file.RecInfo.EMGRMS; % Rms data to test
158 lengthRecording = length(inputData);
159
160 % test the data by each sample
161 for sample = 1:lengthRecording
162     OutputPred(sample,:) = T1C_TestReg([1,inputData(sample,:)], RegCoef);
163 end
164
165 % Plot the prediction
166 plot(OutputPred)
167 % Positive side represents Radio/Extension prediciton
168 % Negative side represents Ulnar/Flexion
169 title(infile(3:end-4))
170 legend('Prediction for Radio/Ulnar','Prediction for Extension/Flexion');
171 set(gca,'FontSize',20);
172 xlabel('Sample [ud]');
173 ylabel('Prediction [%]');
```

Result



Real time implementation

On MyoControl.m:

1. Explain the real time system GUI – [MyoControl.m]
2. Run
App = MyoControl

Real time on VR or prosthesis

1. Collect Data new data by student – [MyoControl.m]
2. Train regressor with student data – [MyoAnalysis.m]
3. Load regressor on real time – [MyoControl.m]
4. Test with the hand or virtual cursor