Deep learning for (deformable) medical image registration

Maureen van Eijnatten



Lecture schedule

Week	Date	Lecturer	Topics	
1	1 Sept.	Maureen	Course introduction; Software demo; Image registration (1)	
	3 Sept.	Maureen	Image registration (2); Geometrical transformations	
2	8 Sept.	Maureen	Point-based registration	
	10 Sept.	Maureen	Intersity-based registration; Evaluation metrics	
3	15 Sept.	Catch-up day (no lecture)		
	17 Sept.	Cornel Zachiu (UMCU)	Guest lecture 1: Image analysis for adaptive radiotherapy	
4	22 Sept.	Mitko	Introduction to CAD; k-NN; Decision trees	
	24 Sept.	Mitko	Generalization and overfitting	
5	29 Sept.	Mitko	Logistic regression; Neural networks	
	1 Oct.	Friso	Convolutional neural networks	
6	6 Oct.	Friso	Deep learning frameworks and applications	
	8 Oct.	Friso	Unsupervised machine learning	
7	13 Oct.	Maureen	Deep learning for deformable image registration	
	15 Oct.	Geert-Jan Rutten (ETZ)	Guest lecture 2: Image analysis in neurosurgery applications	
8	20 Oct	Self-study (no lecture)	Active shape models	
	22 Oct	Self-study (no lecture)	Active shape models	



Outline for today:

- Quick recap of medical image registration
 - Rigid, affine, and non-linear registration models
 - Introduction non-parametric / deformable image registration
- Deep learning
 - Deep iterative registration
 - Supervised methods
 - Unsupervised (optimization-based) methods
- Feedback on project 1
- Question hour and example exam questions

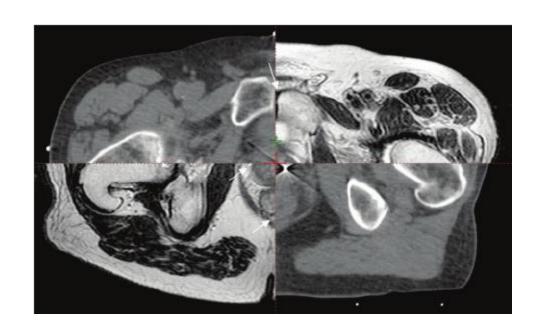
Medical image registration

Why important?

- Multi-modal registration (e.g. CT on MRI)
- Inter-subject (e.g. atlas registration)
- Longitudinal (e.g. treatment evaluation)

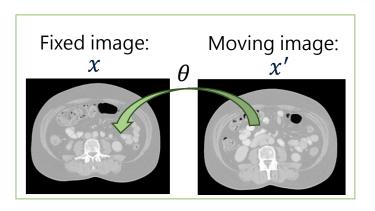
Challenges

- Large 3D volumes
- Accuracy vs. efficiency
- Intensity inhomogeneities and discontinuities
- Outlier rejection





Medical image registration: general "recipe"



Transformation model:

(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure: (e.g. SSD, CC, MI, MSE)

S(x, x')

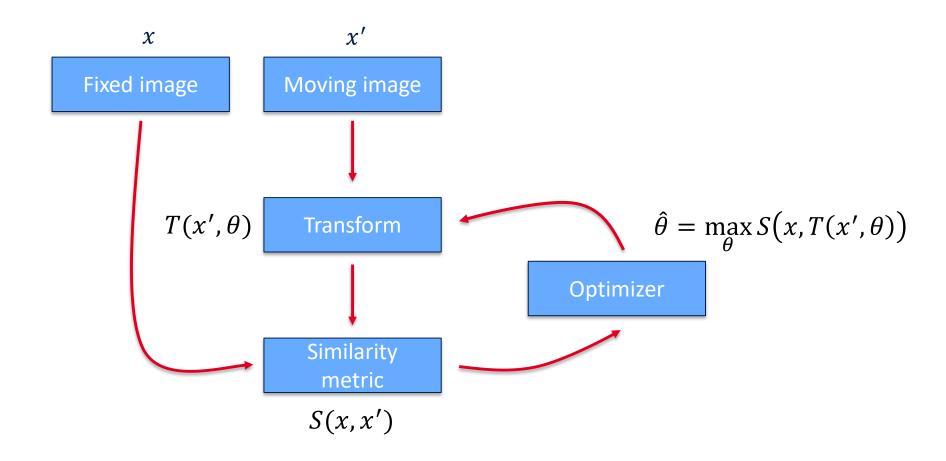
Image registration

Optimization:

$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

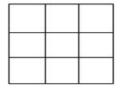


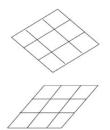
Finding the optimal transformation





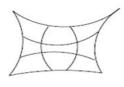
Transformation models





Rigid & Affine

- Point or feature-based (e.g. landmarks, fiducials)
- Intensity-based
- Gradient/edge-based



Non-linear

- Linear or higher order polynomials
- Spline-based

Rigid transformations

$$\mathbf{x}' = \mathbf{R}\mathbf{x} + \mathbf{t}$$

$$\mathbf{t} = egin{bmatrix} t_x \ t_y \end{bmatrix}$$

$$\mathbf{R} = \begin{bmatrix} \cos(\phi) & -\sin(\phi) \\ \sin(\phi) & \cos(\phi) \end{bmatrix}$$

Affine transformations

 $\mathbf{x}' = \mathbf{A}\mathbf{x} + \mathbf{t}$

Translation, rotations and:

$$\mathbf{S} = \begin{bmatrix} s_x & 0 \\ 0 & s_y \end{bmatrix}$$

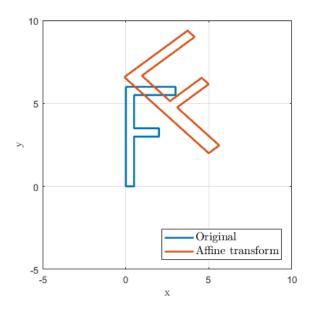
$$\mathbf{H} = \begin{bmatrix} 1 & h_x \\ h_y & 1 \end{bmatrix}$$



Affine transformation (no restriction on the transformation parameters):

$$\begin{bmatrix} x' \\ y' \end{bmatrix} = \begin{bmatrix} a & b \\ c & d \end{bmatrix} \begin{bmatrix} x \\ y \end{bmatrix} + \begin{bmatrix} t_x \\ t_y \end{bmatrix}$$

$$\mathbf{x}' = \mathbf{A}\mathbf{x} + \mathbf{t}$$



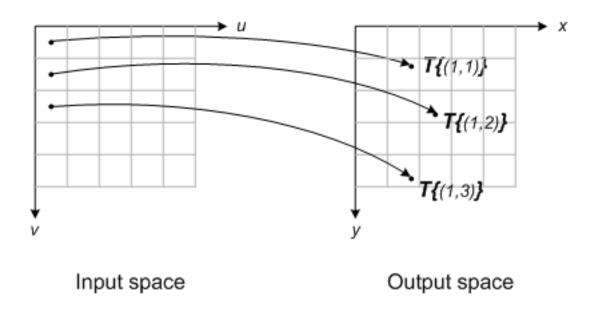
Can be considered as a composition of any combination of rotations, scalings, shearings, reflections + translations.

How many parameters (in 2D)? And in 3D?

3D:
$$\begin{bmatrix} x' \\ y' \\ z' \\ 1 \end{bmatrix} = \begin{bmatrix} a & b & c & t_x \\ d & e & f & t_y \\ g & h & i & t_z \\ 0 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} x \\ y \\ z \\ 1 \end{bmatrix}$$

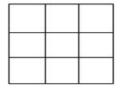


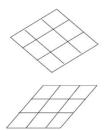
Transforming an image means transforming the spatial coordinates of the pixels.



So far, we have parameterized our transformation model by constraining it to a rigid, affine or non-linear transformation. Is it also possible to define a vector for every pixel?

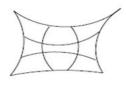
Transformation models





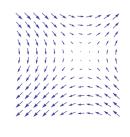
Rigid & Affine

- Point or feature-based (e.g. landmarks, fiducials)
- Intensity-based
- Gradient/edge-based



Non-linear

- Linear or higher order polynomials
- Spline-based

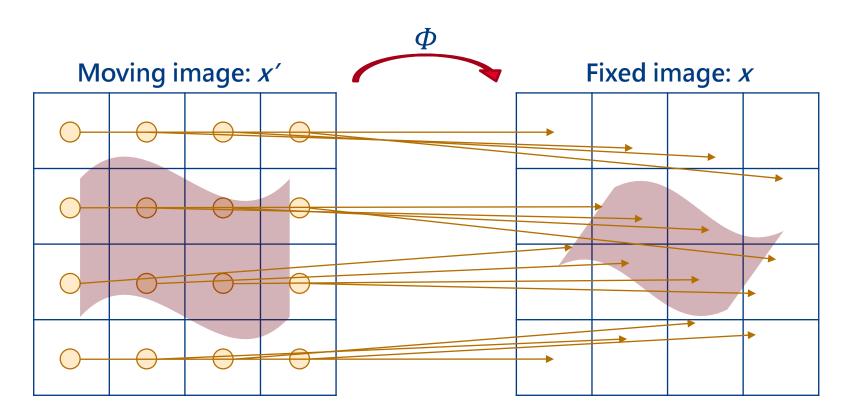


Non-parametric / deformable

Allowing each image element to be displaced arbitrarily



Displacement (vector) field (DVF) = Dense set of vectors representing the displacement in a given spatial domain



Formulation of deformable image registration

Images (fixed image x, moving image x'): $x : \Omega \to \mathbb{R}$

Image domain: $\Omega \to \mathbb{R}^d$, d = 2,3

Regularization moving image: $u' = \underset{u \in H}{\operatorname{arg \, min}} E_D(x, x'(\varphi)) + \lambda E_R(u)$

Difference measure

Deformation: $\varphi = \mathrm{Id} + u$, $\varphi : \Omega \to \mathbb{R}^d$

or point-wise: $\varphi(x) = x + u(x)$

Displacement:

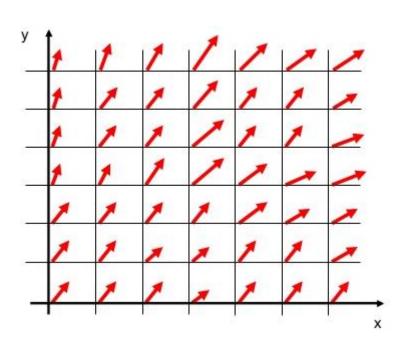
Transformed

$$u:\Omega\to\mathbb{R}^d$$

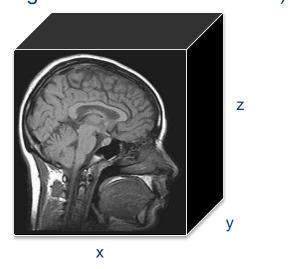
e.g.
$$u = [u_x, u_y, u_z]$$



Deformable image registration: how many free parameters (DOF)?



Typical spatial resolution of a 3D medical image (MRI: e.g. $1.5 \times 1.5 \times 4$ mm³ voxels)



$$DOF = 3*Nx*Ny*Nz (!)$$

Deformable image registration is still a very active area of research, and many different deformable registration models exist:

- Free-form deformation model
- Optical flow
- Demons
- Fluid flow
- Diffeomorphisms
- ...

Note that the details of these models and their implementations are beyond the scope of this course.

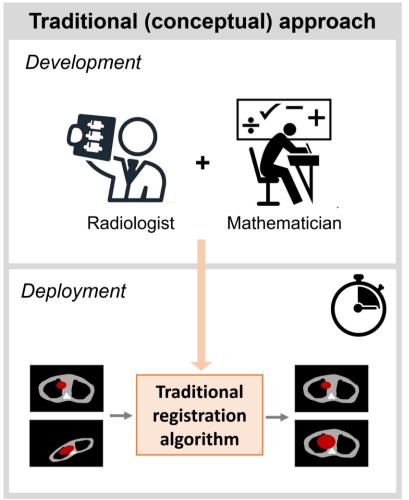
Learning goals of this lecture

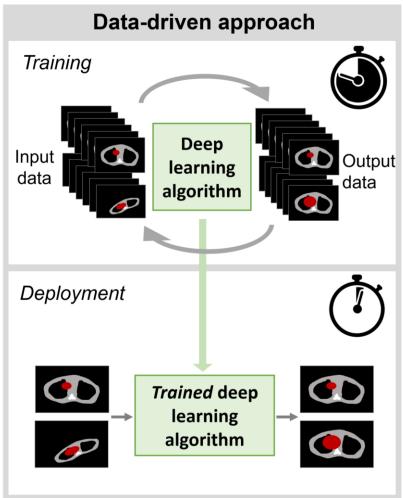
The students should be able to:

- Explain the difference between parametric and non-parametric image registration models
- Formulate deformable image registration as an optimization problem
- Understand displacement vector fields
- Explain the difference between supervised and unsupervised learning
- Understand why deep learning is an interesting technique to solve medical image registration tasks
- Understand the different ways in which deep learning can be used to perform (deformable) image registration



Why focus on deep learning for medical image registration?







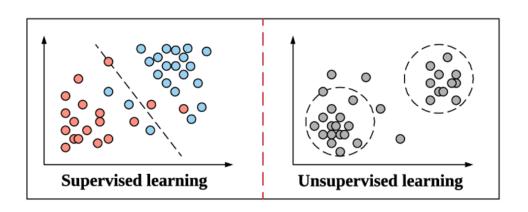
Machine learning – different training strategies

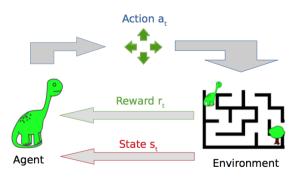
Supervised learning = develop predictive model based on input and output data (i.e., ground truth, "labels")

Examples: <u>classification</u> (e.g., skin lesion classification), <u>regression</u> (segmentation of vessel structures)

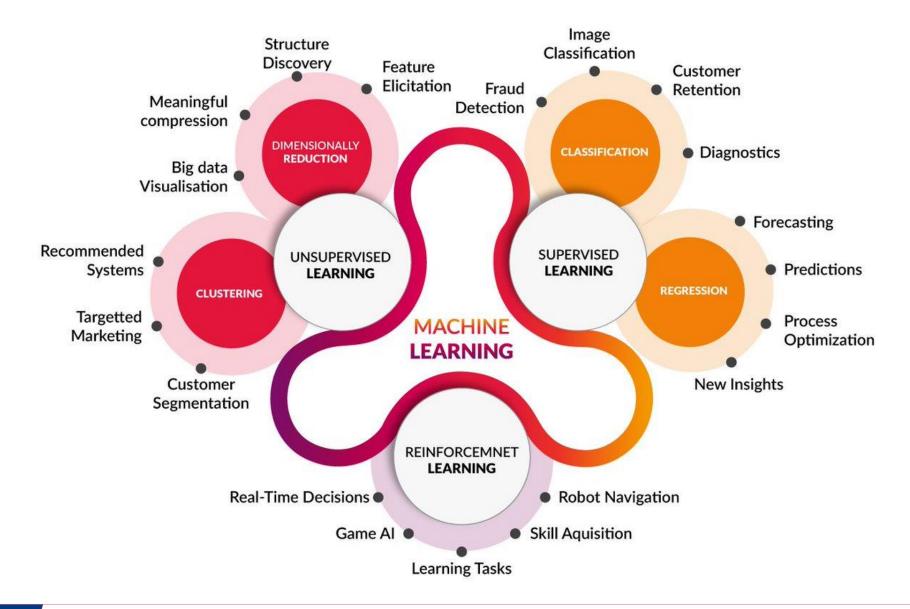
Unsupervised learning = group or interpret data based on input data alone Example: <u>clustering</u> (e.g., k-means)

NB: also semi-supervised learning and reinforcement learning, not part of this course.



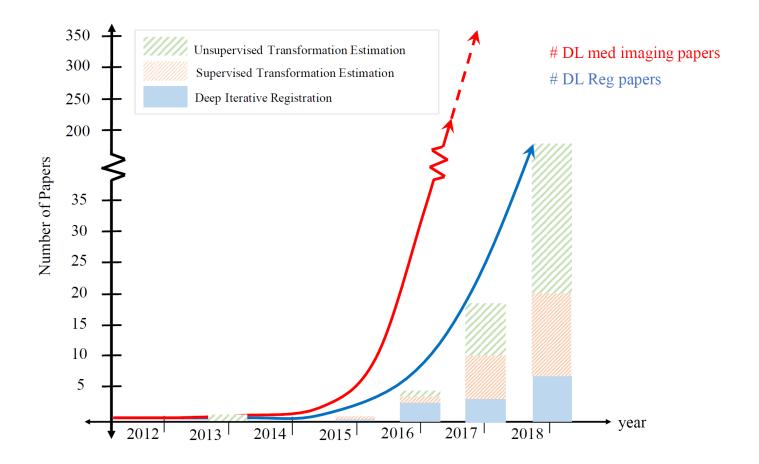


Reinforcement learning



Deep learning-based image registration methods for medical image registration can be subdivided as follows:

- A. Deep iterative registration
- B. Supervised transformation estimation
- C. Unsupervised transformation estimation



A. Deep iterative registration

Use a traditional registration method and learn one component

Automatically extract (learn) similarity features

- Unimodal: Wu et al. (2013) Unsupervised deep feature learning for deformable registration of
 mr brain images (MICCAI); Wu et al. (2016) Scalable high-performance image registration
 framework by unsupervised deep feature representations learning (IEEE Transactions on Biomedical
 Engineering); Eppenhof et al. (2018) Error estimation of deformable image registration of
 pulmonary ct scans using convolutional neural networks (Journal of Medical Imaging)
- Multimodal: Mostly rigid registration; learn a similarity metric to evaluate or register multimodal images using gradient descent. E.g. Cheng et al. (2016&2018) Deep similarity learning for multimodal medical images (MICCAI)

Reinforcement learning

Mostly used for rigid registration

• Low-resolution transformation model for deformable registration

Krebs et al. (2017) Robust non-rigid registration through agent-based action learning (MICCAI)



Where are we in the image registration "recipe"?

Transformation model:

(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure: (e.g. SSD, CC, MI, MSE)

S(x, x')

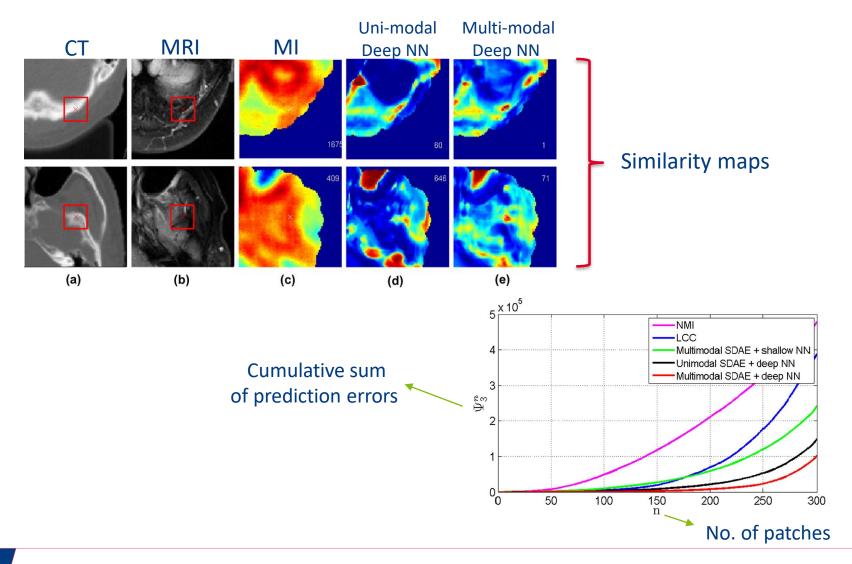
Image registration

Optimization:

$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$



Learned multi-modal feature extraction





Where are we in the image registration "recipe"?

Transformation model:

(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure: (e.g. SSD, CC, MI, MSE)

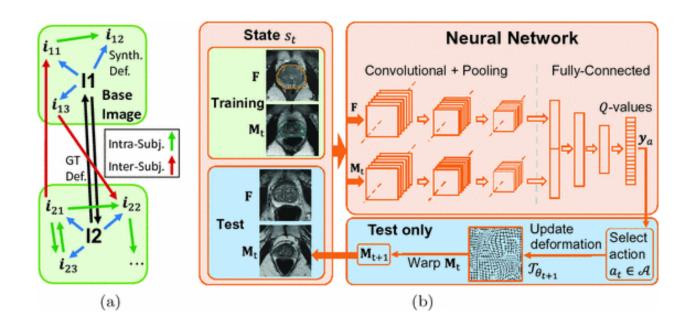
S(x, x')

Image registration

Optimization:

$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

Reinforcement learning for image registration



(a) Training Data Generation: **Synthetic deformations** (blue arrows) and inter-subject GT deformations (black) are used for intra- (green) and inter-subject (red) image pairs for training. (b) Dual-stream network used for Q-value prediction including complete single-stage Markov Decision Process for testing (blue background).

B. Supervised methods

Require many known transformations for training, use ground truth labels to calculate the loss

Fully supervised

2D (FlowNet) vs. 3D approaches (e.g. 3D U-net); mostly patch-based (e.g. 1283)

- Generation of ground truth transformations → many, e.g. Eppenhof et al. (2018)

 Pulmonary ct registration through supervised learning with convolutional neural networks (IEEE trans. on med. imaging)
- Large Deformation Diffeomorphic Metric Mapping (LDDMM) → Yang et al. (2017)

 Quicksilver: Fast Predictive Image Registration a Deep Learning Approach (NeuroImage)

Weakly supervised

Use overlap between segmentations or a similarity metric between M and F combined with ground truth

- MR-US registration
 - CNN → Hu et al. (2018) Weakly-supervised convolutional neural networks for multimodal image registration (Medical Image Analysis)
 - Generative Adversarial Networks (GANs) → Yan et al. (2018) Adversarial image registration with application for mr and trus image fusion (arXiv preprint: 1804.11024)



Supervised learning of the transformation requires a ground truth!

Questions:

- What is the ground truth of an image registration task?
 - Parametric?
 - Non-parametric?
- How can we acquire this?

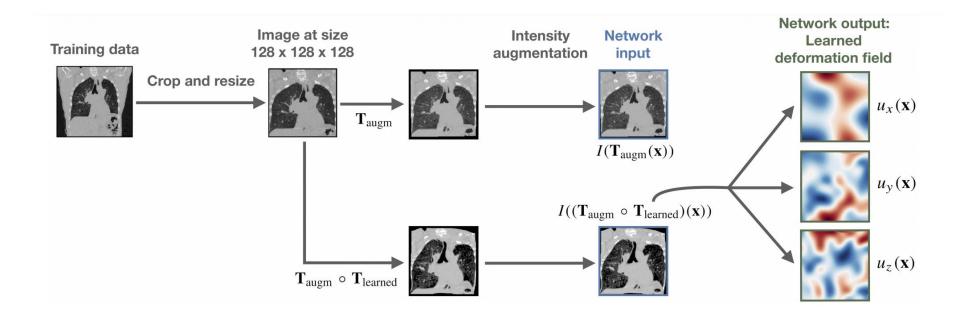


Simulation of displacement vector fields

TABLE I

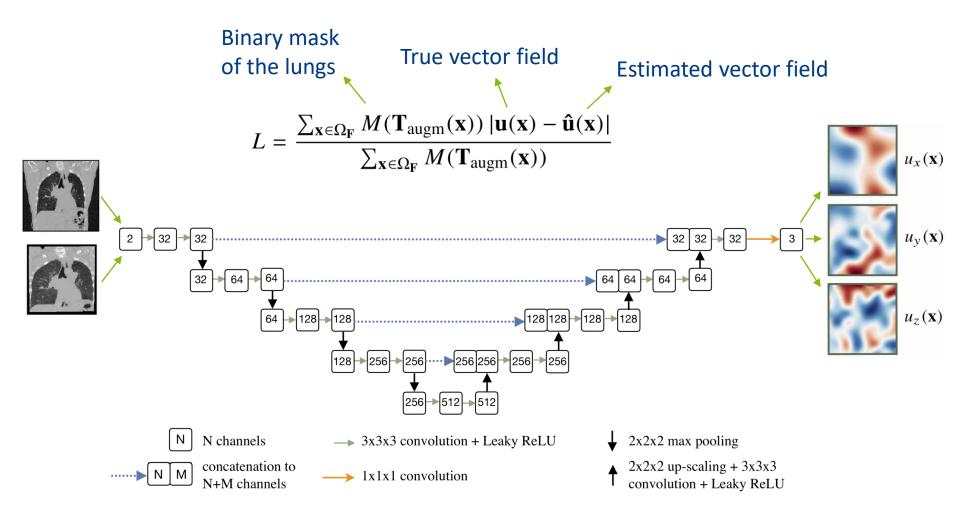
PARAMETERS FOR THE B-SPLINE TRANSFORMATIONS IN THE TRAINING SET. THE GRID SIZE INDICATES THE NUMBER OF GRID POINTS IN EACH DIMENSION. THE DISPLACEMENTS ARE SAMPLED FROM UNIFORM DISTRIBUTIONS IN THE GIVEN RANGES.

		Grid point displacement ranges (voxels)		
T	Grid size	x	у	z
Taugm	$2 \times 2 \times 2$	[-3.2, 3.2]	[-6.4, 6.4]	[-12.8, 12.8]
Tcoarse learned Tfine learned		[-3.2, 3.2] [-3.2, 3.2]	. , ,	[-12.8, 12.8] [-3.2, 3.2]

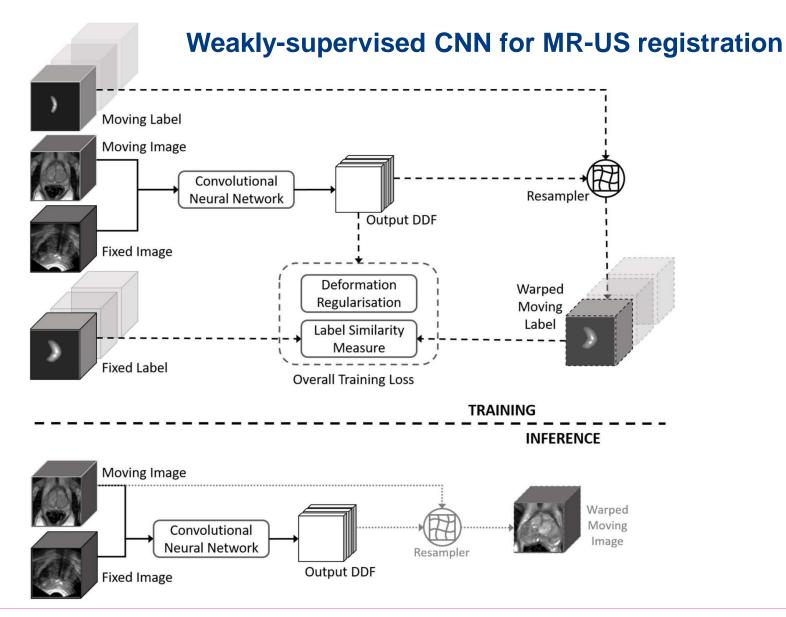




Learning the displacement vector field (Eppenhof & Pluim, 2018)







C. Unsupervised methods

No ground truth needed. Often use a spatial transformer layer.

Variational autoencoders → Krebs et al. (2018) Unsupervised Probabilistic Deformation Modeling for Robust Diffeomorphic Registration. (DLMIA)

Generative Adversarial Networks (GANs) → Tanner et al. (2018)

Generative Adversarial Networks for MR-CT Deformable Image Registration (CVPR) & Hu et al.

(2018) Adversarial Deformation Regularization for Training Image Registration Neural Networks (MICCAI)

Multi-scale methods:

- RegNet → Sokooti et al. (2017) Nonrigid Image Registation Using Multi-scale 3D Convolutional Neural Networks (MICCAI). NB: dual path
- ConvNet → De Vos et al. (2018) A deep learning framework for unsupervised affine and deformable image registration (Medical Image Analysis). NB: chain
- pgCNN → Eppenhof et al. (2019) Progressive Growing Convolutional Networks for Endto-End Deformable Image Registration (SPIE medical imaging)

VoxelMorph (U-net) → Balakrishnan et al. (2019) VoxelMorph: A Learning Framework for Deformable Medical Image Registration (IEEE tran.med.imaging)

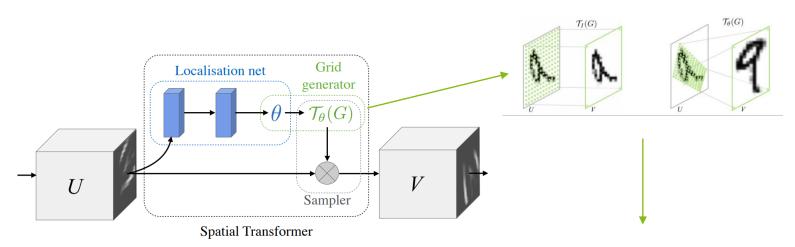
• Cycle-consistent VoxelMorph → Kim et al. (2019) Unsupervised Deformable Image Registration Using Cycle-Consistent CNN (MICCAI)



Spatial transformer networks (Jaderberg et al., NIPS 2015)

Spatial transformer = a learnable module that explicitly allows the spatial manipulation of data within the network

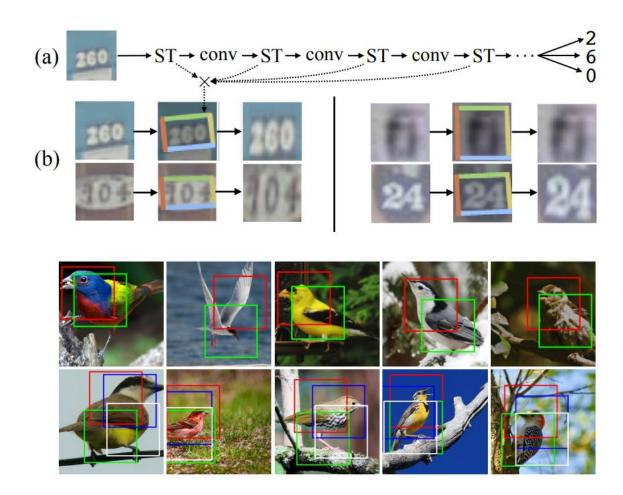
- Differentiable
- Can be inserted into existing convolutional neural networks
- Actively transforms feature maps (conditional on the feature map itself)



Example $T_{\theta}(G)$ for an affine transformation:

$$\begin{pmatrix} x_i^s \\ y_i^s \end{pmatrix} = \mathcal{T}_{\theta}(G_i) = \mathtt{A}_{\theta} \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix} = \begin{bmatrix} \theta_{11} & \theta_{12} & \theta_{13} \\ \theta_{21} & \theta_{22} & \theta_{23} \end{bmatrix} \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix}$$

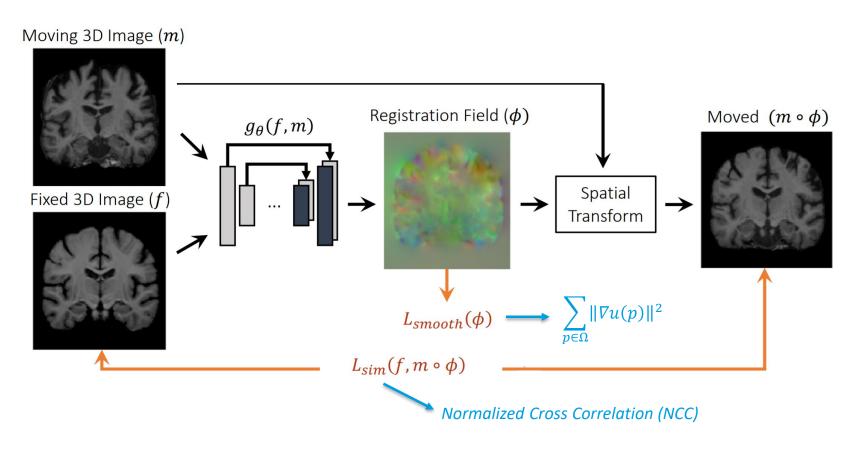
CNNs are in essence not invariant to translation, scale, rotation and more generic warping of the input data





VoxelMorph

Example of a popular unsupervised framework for deformable image registration

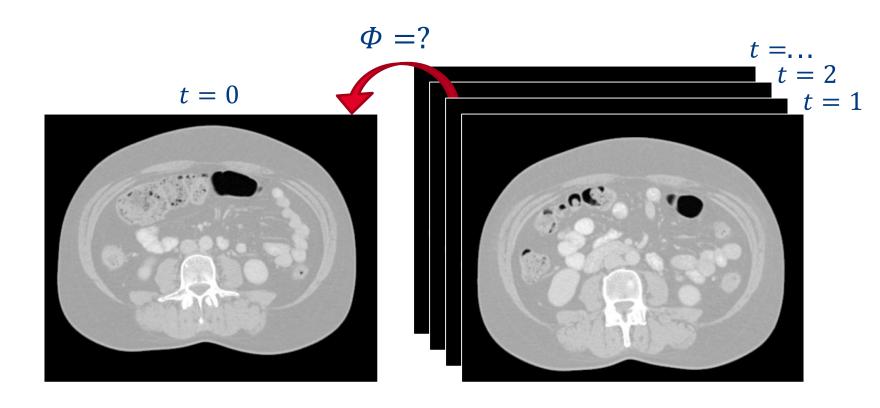


$$\widehat{\Phi} = \underset{\Phi}{\operatorname{argmin}} L_{sim}(f, m \circ \Phi) + \lambda L_{smooth}(\Phi)$$



Example from my own research:

Deformable registration of abdominal CT scans – a longitudinal dataset



Resolution: 512 x 512 x 296; **Voxel dimensions**: 0.7 mm x 0.7 mm x 2 mm



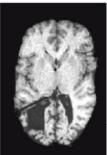
Dataset description

- 140 abdominal and thoracic CT scans of 12 patients with metastasis in the spine
- Gold standard segmentations of vertebrae
- Image registration necessary for reliable response assessment over several time points
- Brain MR image registration relies on skull-stripping techniques
- We developed an automatic region growing algorithm to:
 - Remove patient table
 - Remove non-biological parts (e.g., breast prostheses or clothes) and metal artefacts



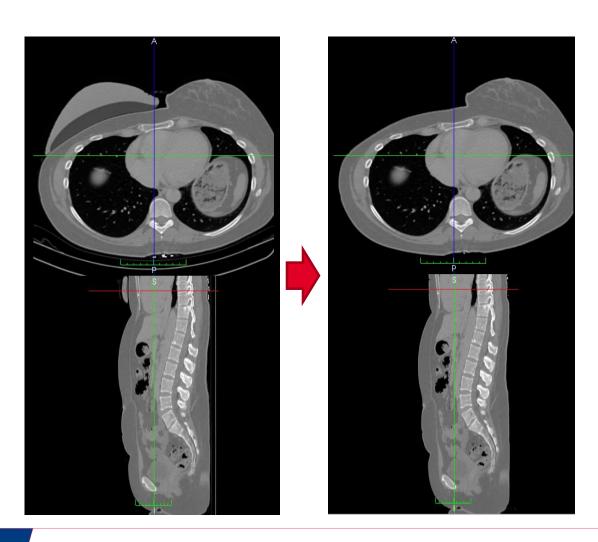




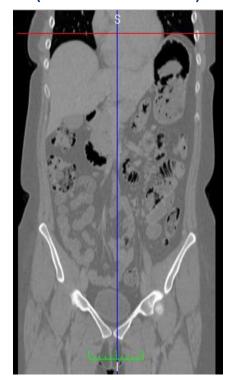




Region growing – example of CT table and breast prosthesis removal



DET 183 – Baseline (abdominal scan)





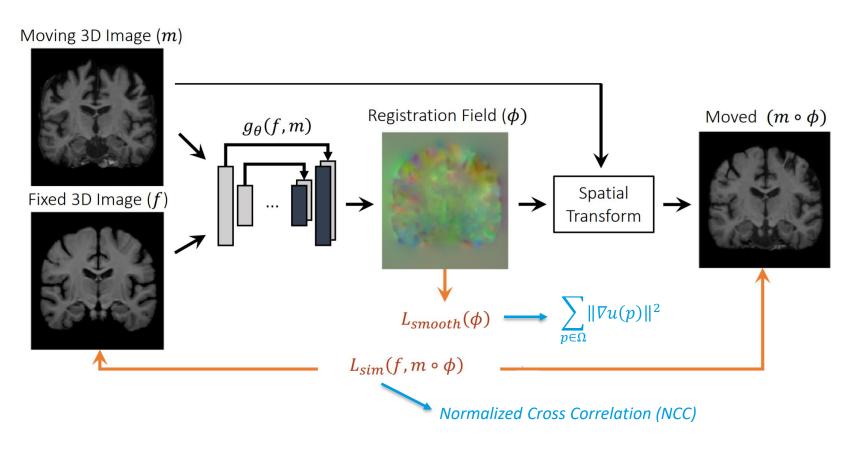
Pre-processing: resampling and affine pre-alignment

Resolution: 160 x 160 x 256; **Voxel dimensions**: 1 mm x 1 mm x 1 mm



VoxelMorph

Example of a popular unsupervised framework for deformable image registration



$$\widehat{\Phi} = \underset{\Phi}{\operatorname{argmin}} L_{sim}(f, m \circ \Phi) + \lambda L_{smooth}(\Phi)$$



Research setting (original VoxelMorph paper):

~6000 brain MRI scans

Real, clinical setting (Addenbrooke's hospital in Cambridge, UK):

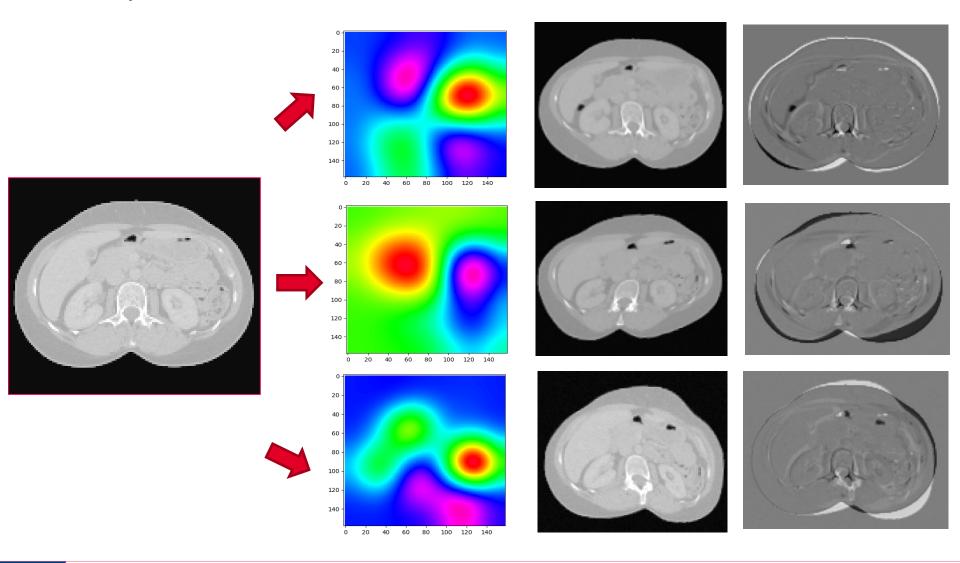
~140 abdominal CT scans

Not enough to train a 3D CNN!

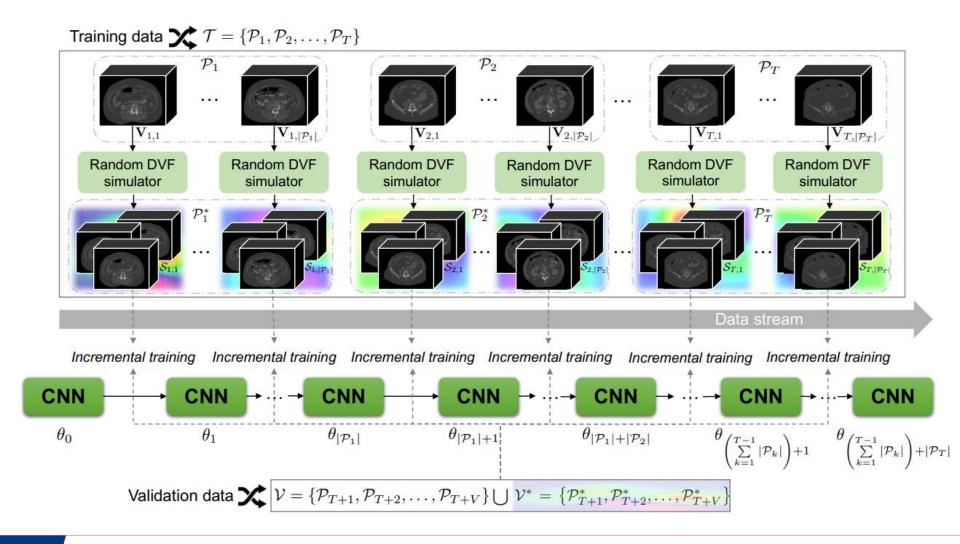
What could we do?



Displacement vector field simulations

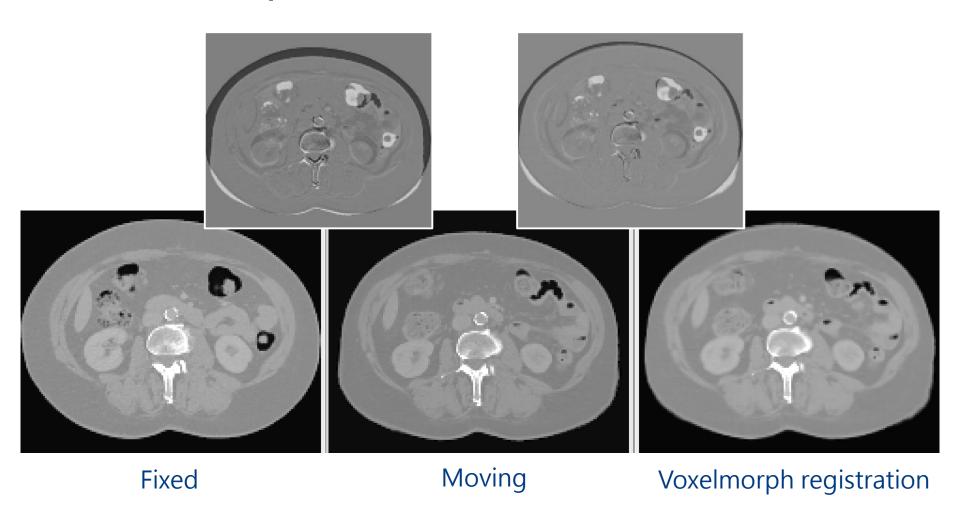


A novel, incremental training strategy (no exam material)



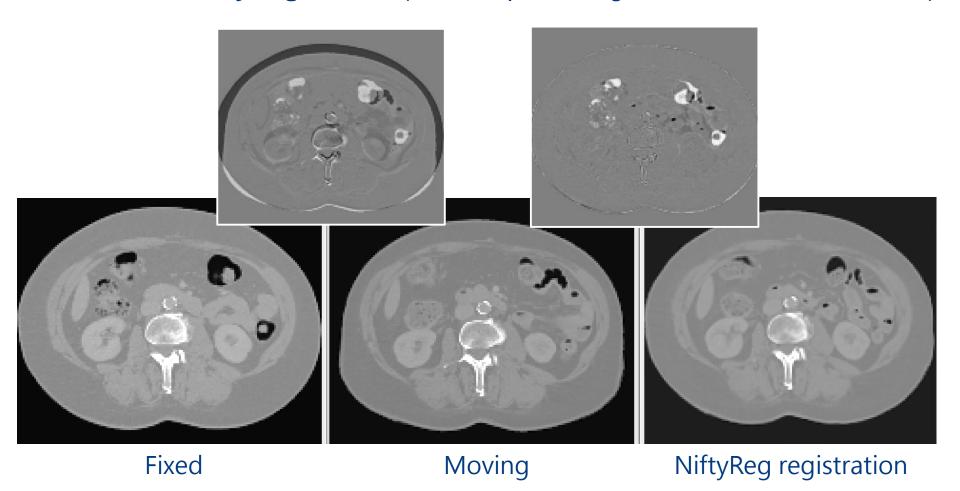


Results: VoxelMorph





Results: the **NiftyReg** toolbox (non-deep learning-based, slow but accurate)



NiftyReg: an open-source software for efficient medical image registration http://cmictig.cs.ucl.ac.uk/wiki/index.php/NiftyReg

Summary

- Parametric vs. non-parametric image registration
- Displacement vector fields
- Formulation of deformable image registration
- Different ways to use deep learning for image registration
 - Deep iterative registration
 - Supervised learning
 - Unsupervised learning
- Disadvantages of deep learning for image registration (performance, # of training data, ground truth, ...)



IMAG/e

Feedback Project 1

General feedback Project 1

- Results: make sure to organize the results well, logical order, caption for each figure!
- Discussion: do the discussed topics directly follow from the results?
- Use references! (NB: scientific writing)
- Reproducibility: e.g. create a notebook that allows others to easily repeat the experiment or run the code

Grades and group-specific feedback have been communicated with all groups via Canvas, if have questions about this, ask your TA (or me).

Preparing for the exam

How can I prepare for the exam?

- (Re)study all exercises and PCA demo (NB: open questions)
 - Answers on Canvas (soon)
- Questions in the lecture slides
- Discussion points CAD by Mitko on Canvas
- Group exercises lecture 2 by Friso ("Deep learning frameworks & applications")
- Some example exam questions on next slides

Question 1

The sequence of transformations that registers a moving to a fixed image is the following: scaling by 0.5 in the x-direction and by 2 in the y-direction, followed by counterclockwise rotation by $\pi/4$ radians.

Which of the following sequence of transformation matrices should be applied to the grid G of the output (transformed) image when performing inverse mapping? Motive your answer.

(a) (c)
$$\begin{bmatrix} \cos(\frac{\pi}{4}) & -\sin(\frac{\pi}{4}) \\ \sin(\frac{\pi}{4}) & \cos(\frac{\pi}{4}) \end{bmatrix} \begin{bmatrix} 2 & 0 \\ 0 & 0.5 \end{bmatrix} \mathbf{G}$$

$$\begin{bmatrix} 2 & 0 \\ 0 & 0.5 \end{bmatrix} \begin{bmatrix} \cos(-\frac{\pi}{4}) & -\sin(-\frac{\pi}{4}) \\ \sin(-\frac{\pi}{4}) & \cos(-\frac{\pi}{4}) \end{bmatrix} \mathbf{G}$$
 (b) (d)
$$\begin{bmatrix} \cos(\frac{\pi}{4}) & -\sin(\frac{\pi}{4}) \\ \sin(\frac{\pi}{4}) & \cos(\frac{\pi}{4}) \end{bmatrix} \begin{bmatrix} 0.5 & 0 \\ 0 & 2 \end{bmatrix} \mathbf{G}$$

$$\begin{bmatrix} 0.5 & 0 \\ \sin(-\frac{\pi}{4}) & \cos(-\frac{\pi}{4}) \\ \sin(-\frac{\pi}{4}) & \cos(-\frac{\pi}{4}) \end{bmatrix} \mathbf{G}$$



[explanation]



Question 2

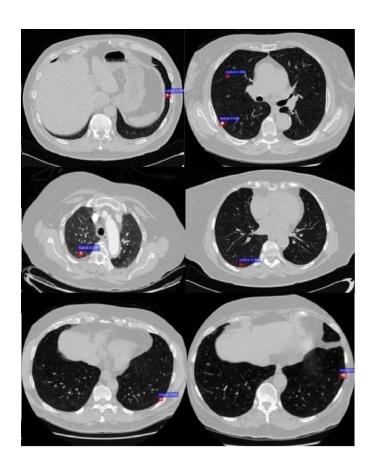
You are given a dataset of 3D MRI scans of the brain. For each scan, you are also given the manually measured brain surface area in cm². You want to use this dataset to train a machine learning model that given a 3D MRI scan as an input will output a prediction of the brain surface area. Is this a classification or a regression problem? Motivate your answer.



Question 3

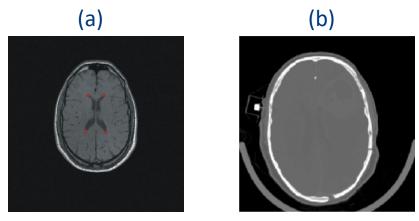
You are asked to develop a convolutional neural network to automatically detect small lung nodules in CT images (see image on the right). The available dataset consists of medical CT images and ground truth segmentations of the nodules delineated by three experienced radiologists. When you visualize the output of the network, the results look promising.

- a) Explain how you would evaluate the performance of your algorithm (use "training set" and "validation set" in your answer).
- b) Which quantitative error metric(s) would you choose to report, and why?
- c) Can you identify factors that influence the performance of your algorithm? Name three.



Some examples of open questions:

- Name two applications of image registration in radiotherapy. Give a short description of every use.
- What type of markers do you see in image (a)? What about image (b)? Give an advantage and disadvantage of using such markers for medical image registration.



- What is the difference between linear and logistic regression?
- What is meant with a receptive field?
- Active shape models → your turn! ☺