

Deep ensemble learning for Alzheimer's disease classification

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ABSTRACT

Ensemble learning uses multiple algorithms to obtain better predictive performance than any single one of its constituent algorithms could. With the growing popularity of deep learning technologies, researchers have started to ensemble these technologies for various purposes. Few, if any, however, have used the deep learning approach as a means to ensemble Alzheimer's disease classification algorithms. This paper presents a deep ensemble learning framework that aims to harness deep learning algorithms to integrate multisource data and tap the 'wisdom of experts'. At the voting layer, two sparse autoencoders are trained for feature learning to reduce the correlation of attributes and diversify the base classifiers ultimately. At the stacking layer, a nonlinear feature-weighted method based on a deep belief network is proposed to rank the base classifiers, which may violate the conditional independence. The neural network is used as a meta classifier. At the optimizing layer, over-sampling and threshold-moving are used to cope with the cost-sensitive problem. Optimized predictions are obtained based on an ensemble of probabilistic predictions by similarity calculation. The proposed deep ensemble learning framework is used for Alzheimer's disease classification. Experiments with the clinical dataset from National Alzheimer's Coordinating Center demonstrate that the classification accuracy of our proposed framework is 4% better than six well-known ensemble approaches, including the standard stacking algorithm as well. Adequate coverage of more accurate diagnostic services can be provided by utilizing the wisdom of averaged physicians. This paper points out a new way to boost the primary care of Alzheimer's disease from the view of machine learning.

1. Introduction

Ensemble learning utilizes a group of decision-making systems that apply various strategies to combine classifiers to improve prediction on new data. Stacking is a well-known approach among the ensembles in which the predictions of a collection of models are given as inputs to a second-level learning algorithm. It has been employed successfully on a wide range of problems, such as chemometrics [1], spam filtering [2], signal processing [3,4], and healthcare [5].

Nevertheless, the correlation of base classifiers is hard to eliminate. Currently, most methods are focusing on diversity among the members of a team of classifiers. For example, different learning algorithms and training data sets have been used for this purpose [6,7]. However, few efforts have been made to reduce the correlation of base classifiers in the second-level algorithm of stacking.

The Restricted Boltzmann Machine (RBM) is a representative example of deep learning, which has become popular in several applications over the last decades, including image recognition [8], bioinformatics [9] and natural language processing [10]. It is a probabilistic model that uses a layer of hidden binary variables or units to model the distribution of a visible layer of variables. As a generative model, it has been used for analyzing different types of data, including labeled or unlabeled images [11], and acoustic data [12]. RBM does not require the independent of input components [11]. It is indeed an advantage to fuse the predictions of base classifiers even they might depend on each other.

Alzheimer's disease (AD) is a chronic neurodegenerative disorder, which makes up more than 60% of all dementia cases [13,14]. Age is the major risk factor for AD. With a rapidly aging world population, diagnosis services in many middle-income countries strive to meet

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actual demand and are mostly confined to tertiary care hospitals in major population centers [15]. Deep learning with some variants has been used for AD prediction in previous works [16,17], but lacked the generalization capability needed for application by medical practitioners owing to insufficient data and the inherent physicians' bias clinical judgments. Making full use of limited resources to improve AD diagnostic accuracy poses a severe challenge in improving healthcare. Hence there is an increasing need for new methods that can enhance the primary care of AD.

The diagnosis of AD is generally based on history-taking, clinical presentation, and behavioral observations. Specialists working in memory clinics sometimes show surprisingly low levels of diagnostic agreement with each other [18], making it hard to obtain objective and reproducible diagnose. Alternatively, more opinions should be sought from primary care services because of the lack of AD specialists in many parts of the world. Therefore, it is vital to find ways to leverage the wisdom of experts better [19]. Our framework is an effective strategy to assist existing or new health professionals, who have insufficient AD-related training, in making a clinical diagnosis.

We regard the clinical decision making of physicians as a learning algorithm that searches a hypothesis space about AD outcome for the best one. Without sufficient data or expertise, the learning algorithms or physicians may derive different AD outcome hypotheses in hypothesis space that would result in the same level of predictive accuracy. By constructing an ensemble of these classifiers or physicians, the algorithm can average decisions and reduce the risk of reliance on the wrong classifier or physician. Many learning algorithms perform local searches for outcome hypotheses that are constrained in local optima. Similarly, physicians may have more expertise in a specific disease, and their diagnoses are often leaned toward what they are most familiar with. An ensemble may provide a better approximation to the real unknown outcome than any individual classifier. Wu et al. combine three different classifiers using weighted and unweighted schemes to improve AD prediction [20]. They use the ¹¹C-PIB PET image data, but the diversity of base classifiers can be further considered. In other words, the base classifiers may depend on each other. There have been recent works on how to combine ensemble learning with deep learning systems to achieve greater prediction accuracy [21,22].

Most of the existing frameworks for AD prediction tend to achieve lower error rates by assuming the same loss for any misclassification. A computer-aided diagnosis system is developed that uses feature ranking and genetic algorithms to analyze structural magnetic resonance imaging data [23]. The conversion of mild cognitive impairment (MCI) to AD is predicted with this system. However, different mistakes may lead to significantly different clinical consequences. For example, failing to detect AD has a more potentially significant consequence than a false positive prediction. Cost-sensitive learning provides a solution to this problem by considering misclassification costs in the learning process [24].

Although using automated computer tools to facilitate medical analysis and prediction is a promising and essential area [25–27], most existing classification methods only use one individual modality of biomarkers for AD prediction, and the data collection process is subject to variability, which may affect the overall classification performance. Voxel wise tissue probability, cortical thickness, and hippocampal volumes are all neuroimaging features often used for AD classification [28–30]. There are, however, also several biological and genetic biomarkers that have been identified as well as being significantly related to increased risk of AD. Different measures provide complementary information, which in combination may significantly increase AD prediction performance. The Uniform Data Set (UDS) stored by the National Alzheimer's Coordinating Center (NACC) includes detailed clinical information of participants, such as cognition outcome, neuropsychological test results, and family history, as well as neuroimaging indices of neurodegeneration [31]. It is a valuable resource that has promoted a wealth of Alzheimer's disease research findings

[32–34].

Based on this multi-dimensional data, we propose a deep ensemble learning framework (DELearning) to leverage the clinical expertise of averaged physicians to obtain more accurate AD prediction. It could be used in primary care settings in which there are limited accesses to specialists. DELearning is a three-layer framework with five stages. Firstly, to fuse multi-source data and reduce the correlation of original features, sparse auto-encoder (SAE) is used for feature learning to construct three feature spaces. Secondly, base classifiers are built by using different learning algorithms and feature spaces. Multiple hypotheses that can be likened to different physician opinions are generated through this kind of manipulation of training data. Thirdly, a new dataset composed of prediction values of classifiers is fed to a Deep Belief Network (DBN), which is used as a stacking method to tackle violations of conditional independence of the base classifiers. Through a contrastive divergence learning procedure [35], DELearning can evaluate different experts and integrate their diagnosis decisions. Fourthly, three Neural Networks (NNs) are constructed based on a back-propagation algorithm, and cost-sensitive methods such as over-sampling and threshold moving. Finally, probabilistic predictions of these models are mapped to a three-dimensional space. Prototypes of different categories are extracted based on mean values. Discrimination is carried out based on the similarity between individuals and prototypes.

The contributions of this paper are as follows:

1. We propose a novel ensemble learning method for AD classification with 4% better than six well-known ensemble approaches, which points out a new way to boost the primary care of Alzheimer's disease.
2. A stacking method is proposed that uses DBN to combine predictions of base classifiers and cope with their dependencies.
3. In our framework, base classifiers are served as surrogates to physicians with different clinical expertise, which can leverage the wisdom of experts and multisource data to make a sound outcome that could be referenced in clinical settings.

The remainder of this paper is organized as follows. Section 2 presents the learning methods of DELearning. Section 3 discusses the empirical results and some observations. Section 4 presents the conclusion of the paper.

2. Methods

This paper interests in two outcomes: probable and possible AD (AD) and non-demented control (NDC). Probable and possible AD is the terminology used in all clinical settings [36]. Suppose we are given a group of samples $\{x_1, \dots, x_i, \dots, x_N\}$ defined on \mathbf{R} , where $1 \leq i \leq N$ the sample size is denoted by N . Each sample has the label $y \in \{+1, -1\}$ representing AD and NDC, respectively. We refer to $X_i = (P_1, \dots, P_j, \dots, P_L)$ are the predictions of L physicians or base classifiers for the sample x_i , where $P_j \in \{+1, -1\}$. Each physician or base classifier L_i gets training samples to predict. All physicians will predict samples. In this paper, we consider the case where there are physicians (simulated by different base classifiers) with different expertise and try to address the question of how to obtain high prediction accuracy based on these circumstances. Refer to Fig. 1 for the framework of DELearning, which composes of three ensemble layers.

First, SAE [37] is used for feature learning to fuse normalized data and construct two feature spaces with a reduced correlation of attributes. Three data spaces are created by adding the normalization of the original data. Next, base classifiers are built by different learning algorithms on these spaces to generate multiple preliminary diagnoses. Thus, the samples are quantified by the predictions of these classifiers.

DBN is used as a meta-classifier to combine the predictions of base classifiers in a weighted manner. It is a probabilistic generative model comprised of multiple Restricted Boltzmann Machines. In some cases,

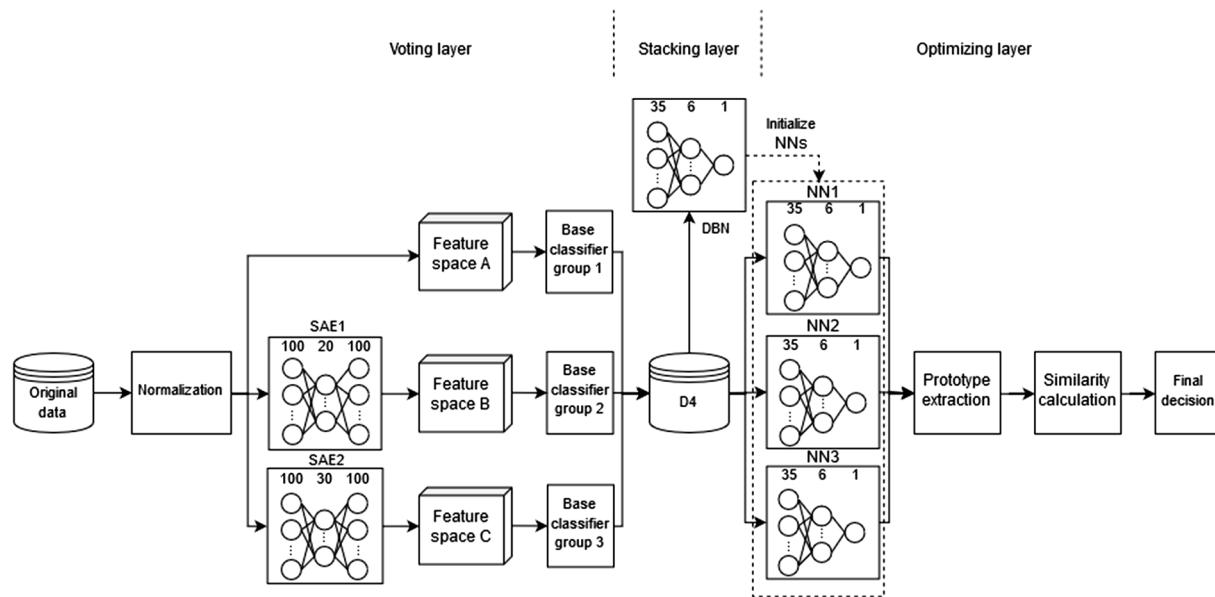


Fig. 1. The framework of DELearning.

while the predictions of some base classifiers may be correlated with each other, the learned features in the hidden layer of RBM can be almost entirely uncorrelated [38]. Therefore, as a probabilistic generative model comprised of multiple RBMs, DBN is trained on the quantized samples as an ensemble method to tackle the dependence of base classifiers.

Three back-propagation NNs are built by the cost-sensitive method and assembled to optimize the predictions. NN₁ is trained on the predictions of base classifiers with threshold moving. NN₂ is trained on the dataset whose distribution is adjusted by over-sampling. NN₃ is initialized as NN₁ and NN₂ by the parameters of the trained DBN model and trained on the same dataset. Then, we map the probabilistic diagnosis of these NNs in a 3-dimensional space and choose the mean values vector as the prototypes of AD and NDC. The similarities between a sample and the two prototypes are calculated by Euclidean distances. Finally, the outcome of the prototype, which is closest to the sample, is selected as the final decision.

2.1. Datasets

The data comes from the National Alzheimer's Coordinating Center [31], which founded in 1999 and has maintained a cumulative database consisting of various types of clinical data such as clinical evaluations, brain MRI imaging, and neuropathology. Many researchers have been making use of this resource to get valuable findings [39]. We extracted 23,165 samples with 100 measures (attributes) from NACC UDS [40]. There are seven groups of measures selected including medical history (MH), Hachinski ischemic score (HIS), cerebrovascular disease (CVD), Unified Parkinson's Disease Rating Scale (UPDRS), Neuropsychiatric Inventory Questionnaire (NPIQ), Geriatric Depression Scale (GDS) and Functional Activities Questionnaire (FAQ). HIS and CVD are separated into two subsets here. Refer to Table 1 for the details.

2.2. Voting layer

Due to the heterogeneous nature of 7 groups of attributes, a single classifier has difficulties in leveraging multisource information sufficiently to obtain a satisfying performance on AD classification no matter the amount of available data. More specifically, the clinical decision boundary that discriminates participants from different outcomes may be linear for some attributes while non-linear for another part. It may lie outside the space of functions that can be implemented

by the chosen classifier. Even though a single classifier could achieve satisfying classification performance on the available data, it might not generalize for other data sources.

Three feature spaces are constructed by normalizing original data and two sparse autoencoders. Sixteen classification algorithms are trained on them to forming three base classifier groups to increase the generalization ability and diversify the decision boundaries. These classification algorithms consist of Bayes Network, Naive Bayes, J48, Hoeffding tree, REPTree, Filtered Classifier, Iterative Classifier Optimizer, Logistic Regression, LogitBoost, Multilayer Perception, Stacking, Random Committee, Random Forest, Random Subspace, AdaBoostM1, and Voted Perceptron. The prediction results from thirty-five classifiers selected with better performance are combined and fed into the next layer.

This section briefly illustrates three classification algorithms. Logistic Regression is a well-behaved classification algorithm, specially when the features to be studied can be treated as roughly linear, or the problem is linearly separable [41]. As a commonly used classifier, it can also deal with nonlinear problems through discretization and mapping of features. This discriminative model is also robust to noise and can avoid overfitting by using L1 or L2 regularization.

Tree ensembles like Random Forests are a combination of a bunch of decision trees [42]. One dominant advantage of tree ensemble is that they do not presume linear features for data. So, they are quite suitable for handling certain features.

Naive Bayes classifier is a probabilistic model based on Bayes theorem that can simplify learning by assuming that features are independent given class [43]. In the case of conditional independence, less data is needed in training a naive Bayes classifier due to that often converge faster than discriminative models such as Logistic Regression. Although this assumption is often impractical in the real world, Naive Bayes classifier still performs better in practice.

Various indicators such as Q-statistic and "difficulty" θ have been discussed for quantitative assessment of diversity [44]. Q-statistic is a measure to evaluate the similarity of two classifiers' predictions. It is formulated as

$$Q_{ij} = \frac{N_{11}N_{00} - N_{01}N_{10}}{N_{11}N_{00} + N_{01}N_{10}} \quad (1)$$

of which N_{ab} is the number of samples where the classifier i has outcome a , and the classifier j has outcome b , where a and b could have value 0 (when the classifier predicts the wrong class) or 1 (when the

Table 1

Seven groups of measures selected from NACC UDS.

Groups	Measures
MH	CVHATT, CVAFIB, CVANGIO, CVBYPASS, CVPACE, CVCHF, CVOTHR, CBSTROKE, CBTIA, CBOTHR, PD, SEIZURES, TRAUMBRF, HYPERTEN, HYPERCHO, DIABETES, B12DEF, THYROID, INCONTU, INCONT
HIS	ABRUP, STEPWISE, SOMATIC, EMOT, HXHYPER, HXSTROKE, FOCLSYM, FOCLSIGN, HACHIN
CVD	CVDVOG, STROKCOG, CVDIMAG, CVDIMAG1, CVDIMAG2, CVDIMAG3, CVDIMAG4
UPDRS	SPEECH, FACEXP, TRESTFAC, TRESTLHD, TRESTLFT, TRESTRFT, TRACTLHD, RIGDNECK, RIGDUPRT, RIGDULF, RIGDLORT, RIGDLOLF, TAPSRT, TAPSLF, HANDMOVR, HANDMVL, HANDALTL, LEGRT, LEGLF, ARISING, POSTURE, GAIT, POSSTAB, BRADYKIN
NPIQ	DEL, HALL, AGIT, DEPD, ANX, ELAT, APA, DISN, IRR, MOT, NITE, APP
GDS	SATIS, DROPACT, EMPTY, BORED, SPIRITS, AFRAID, HAPPY, HELPLESS, STAYHOME, MEMPROB, WONDRFUL, WRTHLESS, ENERGY, HOPELESS, BETTER
FAQ	BILLS, TAXES, SHOPPING, GAMES, STOVE, MEALPREP, EVENTS, PAYATTN, REMDATES, TRAVEL
Total number	samples: 23165; outcomes: 2; measures: 100

classifier predicts the correct class for the sample).

As to multiple classifiers' diversity assessment, the difficulty θ is used and defined as the variance of a discrete random variable X , which denotes the proportion of base classifiers that correctly classify a participant drawn randomly from the original training data.

We can treat the trained base classifiers as physicians from different fields with different clinical expertise because of these diversities. For a participant, the prediction of a classifier is equivalent to the diagnosis result of the corresponding physician.

In addition to different learning algorithms, resampling of the training data is another way to increase the diversity of base classifiers. The clinical measures extracted from NACC are sparse, which affects the performance of some classifiers. To improve diversity and obtain high-level feature representation, two SAEs are used in the voting layer to automatically learn different feature spaces defined by the activations of their hidden nodes. We take SAE with a three-layer symmetrical structure including an input layer, a hidden layer, and an output layer. Seven node groups in the input layer consists of 100 nodes corresponding to measures in Table 1. The suitable number of nodes in the hidden layer can be selected according to reconstruction error to determine the dimensions of feature spaces. The activation values of hidden nodes are extracted as high-level features. Refer to Fig. 2 for the details of the SAE structure.

Suppose the activation function of hidden units is the sigmoid function, the average activation of hidden unit j over n samples is denoted as

$$\hat{\rho}_j = \frac{1}{n} \sum_{i=1}^n a_j(x^{(i)}) \quad (2)$$

where $a_j(x^{(i)})$ is the activation function of the hidden unit j given a sample $x^{(i)}$. A sparse representation is used to represent the input data better. The constraint $\hat{\rho}_j = \rho$ is enforced to make hidden unit's activation mostly near the sparsity parameter ρ whose typical value close to 0.

To satisfy the constraint, we apply Kullback-Leibler (KL) divergence to optimization objective J (reconstruction error), serving as a sparsity penalty term. It is formulated as follows [45].

$$J_{SAE}(W, b) = J(W, b) + \beta \sum_{j=1}^n KL(\rho || \hat{\rho}_j) \quad (3)$$

where W , b is weight and bias, respectively, $KL(\rho || \hat{\rho}_j) = (\rho \log \frac{\rho}{\hat{\rho}_j} + (1 - \rho) \frac{1 - \rho}{1 - \hat{\rho}_j})$, n is the number of hidden units.

The most crucial advantage of feature learning by SAE is that the correlation of transformed features is significantly reduced. Thereby, trained on these feature spaces, the diversity of base classifiers can be further improved.

2.3. Stacking layer

Stacking is an ensemble technique in which the predictions of a

group of predictive models are combined through other learning models to generate a final output. In our stacking layer, the predictions of base classifiers from the voting layer are combined as inputs to the DBN that composed of two RBMs. RBM is a probabilistic model that uses variables of a hidden layer to model the distribution of observed data. Typically, an RBM is trained in an unsupervised manner to model the distribution of the inputs. The most outstanding strength of RBM is that the hidden units are conditionally independent, given the visible units [11]. It can learn the abstract representation from the predictions of base classifiers. As shown in Fig. 3, we train the DBN that consists of 35 nodes in the input layer, which corresponding to base classifiers with better performance selected, six nodes in the first hidden layer, and one node in the second hidden layer on the predictions of base classifiers. After the pre-training of RBMs in a layer-wise manner, the back-propagation learning algorithm is adopted for fine-tuning based on mean square error (MSE). The parameters of the trained DBN are used to initialize three neural networks with the same structure in the next layer, which reduces the effect of correlation from base classifiers' predictions.

2.4. Optimizing layer

One challenge in AD diagnosis is that the number of patients is fewer than healthy people in primary care settings. The cost of a missed diagnosis is higher than that of misdiagnosis under this circumstance. Cost-sensitive learning is a suitable tool for learning both from imbalanced datasets and unequal costs [24]. Based on Ref. [6], DE-Learning adapts over-sampling, threshold moving as cost-sensitive strategies to train NNs and assemble their probabilistic predictions.

In DELearning, there are two diagnosing outcomes for a participant, i.e., $y \in \{AD, NDC\}$. The participant number corresponding to these two outcomes is N_i and N_j respectively. $Cost[i, j]$ ($i, j \in \{1, 2\}$) denotes the cost of a participant that belongs to the i^{th} outcome misdiagnosing as the j^{th} outcome (if the diagnosis is right then $Cost[i, i] = 0$). Under binary classification circumstances, it is clear that the cost of the i^{th} outcome $Cost[i]$ is equal to $Cost[i, j](i \neq j)$. The cost matrix can be represented as

$$\begin{bmatrix} 0 & Cost[2, 1] \\ Cost[1, 2] & 0 \end{bmatrix} \quad (4)$$

In order to solve the problem of unbalanced data and categories, we consider adopting oversampling for categories with fewer data. Suppose $N_i < N_j$, the i^{th} outcome will have N_i^* individuals after resampling. It can be computed as follows.

$$N_i^* = |\varphi \cdot N_j| \quad (5)$$

where $\varphi = \frac{Cost[i]}{Cost[j]}$ is called the coefficient of cost. The ranges of this parameter should fall into $N_i^* > N_i$, and the category not be overfitted. Thus $(N_i^* - N_i)$ participants can be resampled for the i^{th} category with random replacement.

Since under-sampling discards potentially useful training samples,

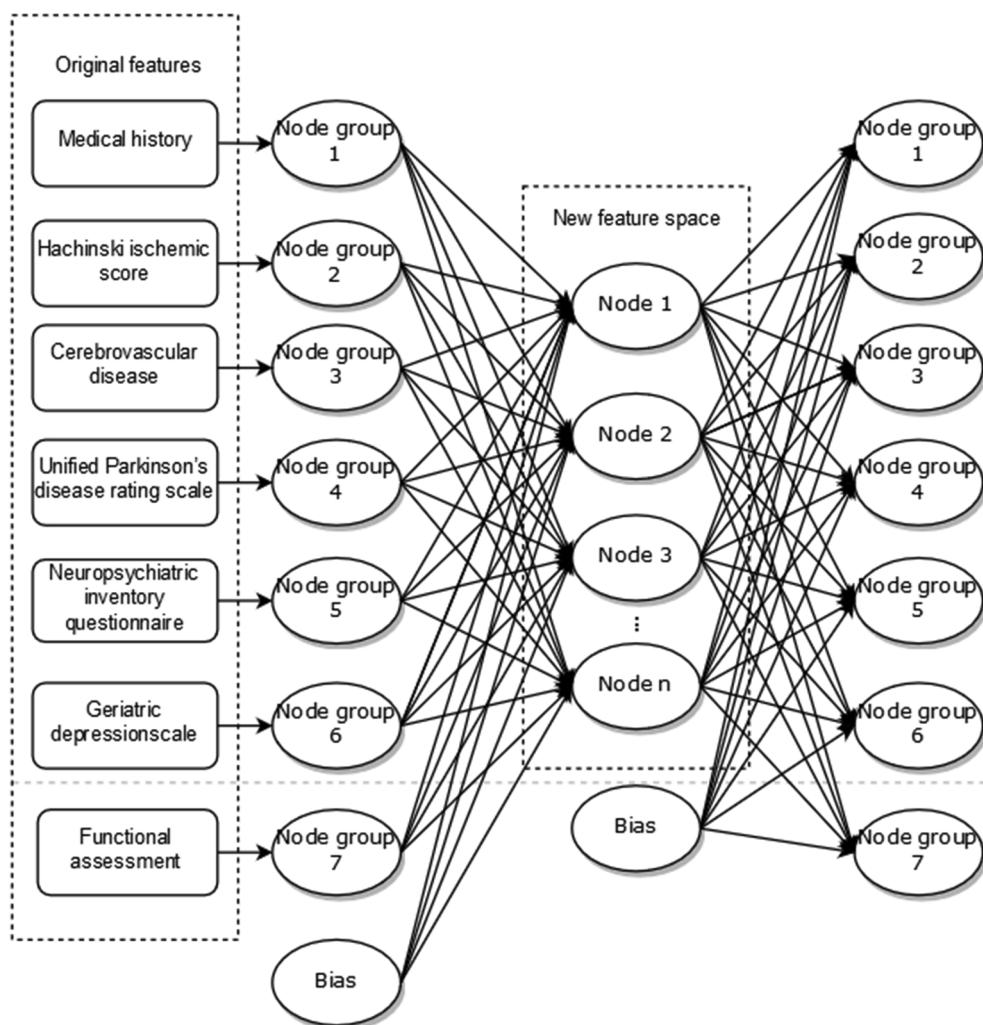


Fig. 2. The structure of SAE.

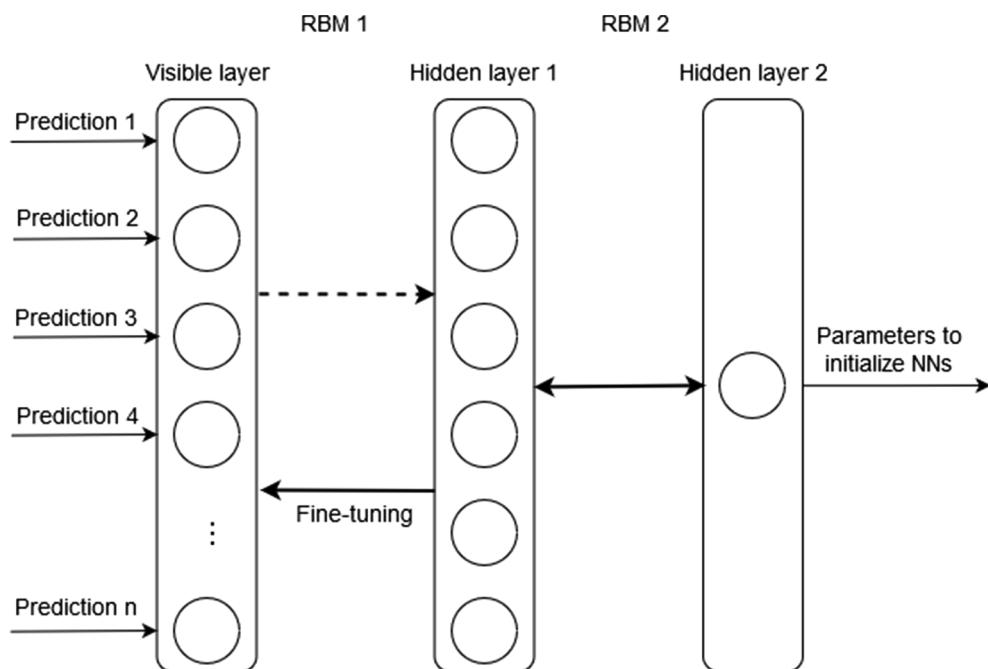


Fig. 3. Stacking layer of DELearning with DBN.

the performance of the resulting classifier may be degraded. DELearning uses over-sampling for training NN in the optimizing layer.

Besides over-sampling, we also use threshold moving to adjust the output unit in NN toward an inexpensive outcome so that participants with higher misclassification costs will be easily identified.

Suppose O_i and O_i^* are denoted as the output of NN in optimizing layer with or without threshold moving, the normalized real value O_i^* can be adjusted in DELearning as follows.

$$O_i^* = \frac{Cost[i]}{Cost[i] + Cost[j]} O_i, i \neq j \quad (6)$$

After training DBN in the stacking layer, the parameters and structure are used to initialize three neural networks in the optimizing layer. NN_1 is trained with threshold-moving and NN_2 with over-sampling, respectively, on the predictions of base classifiers. NN_3 is also trained directly on these predictions. The real-value outputs of these three NNs are combined to form prototypes for each category. The Euclidean distances are computed between samples and the two prototypes. The category with the smallest distance is selected as the final prediction result for the samples.

The DELearning algorithm is shown in Table 2.

2.5. Performance measures

A confusion matrix that contains the actual outcome and predicted outcome is used to evaluate the performance of AD classification. Table 3 presents the confusion matrix for AD classification with two outcomes. TP is the number of AD patients that are correctly classified as AD. FP is the number of NDC participants that are diagnosed as AD. FN is the number of AD patients that are incorrectly classified as NDC. TN is the number of NDC participants that are classified correctly. We use the following four measures to evaluate DELearning as well as all the base classifiers. The statistically significant comparison of performances of DELearning and benchmarks are performed by using McNemar's test [46]. The adjustment for multiple comparisons is performed using Bonferroni correction [47].

Accuracy is the proportion of all participants that are correctly classified as either AD or NDC. It is formulated as the following:

$$Accuracy = \frac{TP + TN}{TP + FP + FN + TN} \times 100\% \quad (7)$$

Precision denotes the proportion of predicted AD cases that are real

Table 2
Proposed DELearning algorithm.

Input: Samples D with clinical measures and outcomes;
Output: Prediction of AD or NDC

Voting Layer:

1. Normalize the original data set D, get D_1 .
2. Train two SAEs on D_1 .
3. Derive the optimal structure of SAEs based on MSE.
4. Construct data sets D_2 and D_3 by extracting activation values of hidden layers in SAEs.

Stacking Layer:

5. Train base classifiers on D_1 , D_2 , and D_3 .
6. Generate data set D_4 consisting of the predictions of all base classifiers.

Optimizing Layer:

7. Train DBN on D_4 to stack the predictions of base classifiers.
8. Generate the parameters and structures of the trained DBN.
9. Initialize three neural networks NN_1 , NN_2 , and NN_3 with the parameters and structures of DBN.
10. Train NN_1 with threshold-moving on D_4 .
11. Train NN_2 with over-sampling on D_4 .
12. Train NN_3 on D_4 .
13. Generate predictions of NN_1 , NN_2 , NN_3 .
14. Generate prototypes for AD and NDC.
15. Calculate the similarity between samples and prototypes.
16. Make a final decision according to similarity.

Table 3
Confusion matrix for AD prediction.

		Predicted outcome	
		AD	NDC
Actual outcome	AD	TP	FN
	NDC	FP	TN

AD patients.

$$Precision = \frac{TP}{TP + FP} \times 100\% \quad (8)$$

The recall is the proportion of AD patients that are correctly classified. It reflects the ability of a classifier to recognize positive examples. In a medical context, recall is regarded as a more primary measure than precision [48], as the aim is to identify all real positive cases.

$$Recall = \frac{TP}{TP + FN} \times 100\% \quad (9)$$

F1-measure provides a way to combine precision and recall into a single measure with no imbalanced manner, which can be formulated as follows:

$$F1\text{-measure} = 2 \times \frac{Precision \times Recall}{Precision + Recall} \times 100\% \quad (10)$$

3. Results and discussion

The original dataset is randomly split into three subsets, namely subset1 (50%), subset2 (30%), and subset3 (20%). Subset1 (50%) is used to select the base classifiers. Subset1 and subset2 are used as the training set (80%). Subset3 is used as the testing set (20%). In the training process, subset1 is used to train and further select the base classifiers. Tables 4–7 shows the performance of classifiers on subset1 by 5-fold cross-validation. Based on it, the classifiers with better performance are incorporated into our model as the base classifiers. Then, the base classifiers make predictions on the training set (subset1 and subset2). These predictions are used to train DBN as well as three NNs that initialized by the parameters of DBN. The prototypes of NDC and AD are extracted based on the predictions of three NNs. In the testing phase, it is an end-to-end evaluation which is carried out on the testing set (subset3), which successively experienced SAEs, base classifiers,

Table 4

Accuracy of base classifiers in three feature spaces. (A) normalized original space, (B) 20-dimensional space learned by SAE, (C) 30-dimensional space learned by SAE.

Classifier	Feature space		
	A	B	C
Bayes Nets	75.6%	71.4%	72.6%
Filtered Classifier	79.2%	75.4%	75.3%
Hoeffding Tree	78.5%	76.0%	74.7%
Iterative Classifier Optimizer	79.9%	75.3%	76.3%
J48	79.1%	75.1%	75.8%
Logistic Regression	80.4%	77.2%	78.0%
LogitBoost	79.9%	75.3%	76.3%
Random Committee	82.7%	75.6%	75.4%
Random Forest	81.7%	83.9%	78.4%
Random SubSpace	81.8%	76.1%	77.4%
REPTree	80.4%	76.0%	75.9%
AdaBoostM1	76.2%	74.4%	75.5%
Multilayer Perception	80.5%	79.7%	80.1%
Naïve Bayes	72.1%	71.5%	73.6%
Stacking	63.1%	62.6%	63.1%
Voted Perceptron	78.5%	77.4%	76.4%

Table 5

The precision of base classifiers in three feature spaces. (A) normalized original space, (B) 20-dimensional space learned by SAE, (C) 30-dimensional space learned by SAE.

Classifier	Feature space		
	A	B	C
Bayes Nets	76.1%	73.9%	73.1%
Filtered Classifier	79.1%	75.5%	75.1%
Hoeffding Tree	79.1%	76.1%	74.6%
Iterative Classifier Optimizer	79.8%	76.1%	76.4%
J48	78.9%	74.7%	76.2%
Logistic Regression	80.2%	77.3%	78.0%
LogitBoost	80.1%	76.1%	76.4%
Random Committee	82.7%	75.2%	75.1%
Random Forest	80.1%	80.9%	78.1%
Random SubSpace	81.8%	75.8%	77.2%
REPTree	80.4%	76.3%	76.0%
AdaBoostM1	78.5%	77.1%	75.8%
Multilayer Perception	80.3%	79.5%	78.3%
Naive Bayes	71.5%	73.8%	75.4%
Stacking	60.2%	61.3%	60.5%
Voted Perceptron	78.3%	77.5%	78.1%

Table 6

Recall rate of base classifiers in three feature spaces. (A) normalized original space, (B) 20-dimensional space learned by SAE, (C) 30-dimensional space learned by SAE.

Classifier	Feature space		
	A	B	C
Bayes Nets	75.6%	71.4%	72.3%
Filtered Classifier	79.3%	75.4%	75.4%
Hoeffding Tree	78.5%	76.0%	74.7%
Iterative Classifier Optimizer	79.9%	75.4%	76.3%
J48	79.1%	75.1%	75.8%
Logistic Regression	80.5%	77.3%	78.1%
LogitBoost	79.9%	75.4%	76.3%
Random Committee	82.8%	75.6%	75.5%
Random Forest	82.8%	84.9%	77.5%
Random SubSpace	81.9%	76.2%	77.4%
REPTree	80.4%	76.0%	75.9%
AdaBoostM1	76.1%	74.5%	75.5%
Multilayer Perception	80.4%	79.8%	79.9%
Naive Bayes	72.2%	71.6%	73.6%
Stacking	64.2%	62.7%	62.8%
Voted Perceptron	78.0%	77.4%	77.9%

NNs, and similarity calculation to generate the final prediction result.

3.1. Feature learning

DELearning utilizes SAE as a feature learning method to obtain more discriminative features compared with the original set. In order to determine the optimal dimension of transformed space and reduce data correlation, we trained three-layer SAE models with 100 input units and 10, 20, 30 hidden units, respectively. The activation function was sigmoid. Obvious biases and weights were initialized to zero and random numbers sampled from a normal distribution with zero mean and standard deviation 1. Momentum was set to 0.5. The model was trained for 100 epochs. As shown in Fig. 4, the MSE of models with 20, 30 hidden units are much smaller than the model with 10 hidden units. Considering lower dimensions of data selection in situations of limited reduction of MSE, the number of hidden units of SAEs is set to 20 and 30 for the transformation of feature space.

As shown in Fig. 5, we compared the performance of SAE with commonly used sparsity parameter $\rho=0.01, 0.05, 0.1$, and 0.15, respectively. It can be seen that the best performance at $\rho=0.05$. So, we set $\rho=0.05$ in DELearning.

Table 7

F1-measure of base classifiers in three feature spaces. (A) normalized original space, (B) 20-dimensional space learned by SAE, (C) 30-dimensional space learned by SAE.

Classifier	Feature space		
	A	B	C
Bayes Nets	75.8%	71.9%	72.1%
Filtered Classifier	79.2%	75.4%	75.2%
Hoeffding Tree	78.7%	76.0%	73.5%
Iterative Classifier Optimizer	79.9%	75.6%	76.4%
J48	79.0%	74.7%	76.0%
Logistic Regression	80.2%	77.3%	78.0%
LogitBoost	79.9%	75.6%	76.4%
Random Committee	82.7%	75.3%	75.1%
Random Forest	82.7%	82.9%	78.4%
Random SubSpace	81.8%	75.8%	77.3%
REPTree	80.4%	76.1%	75.9%
AdaBoostM1	76.1%	74.9%	75.6%
Multilayer Perception	80.3%	79.5%	79.8%
Naive Bayes	71.4%	72.0%	74.0%
Stacking	62.2%	60.3%	60.6%
Voted Perceptron	78.1%	77.5%	77.8%

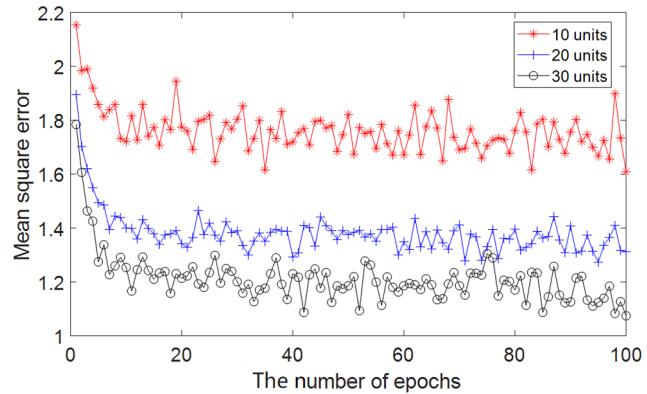


Fig. 4. The performance comparison of SAEs with 10, 20, 30 hidden units. The x-axis indicates the number of epochs, and the y-axis indicates the MSE with the corresponding epoch.

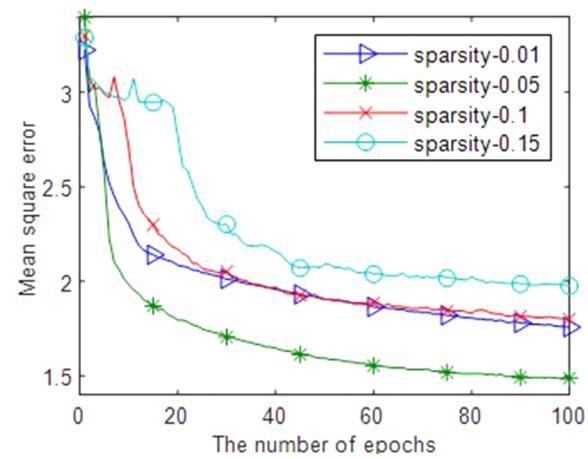


Fig. 5. The MSE of SAE with specific parameter ρ .

The samples after feature transformation are easier to distinguish from their categories. Fig. 6 presents 100 participants randomly selected from three feature spaces. In the original space, most features of participants with different outcomes are overlap with each other. With the transformed features, the boundary between AD and NDC is relatively obvious, which intuitively indicates that the dimension of

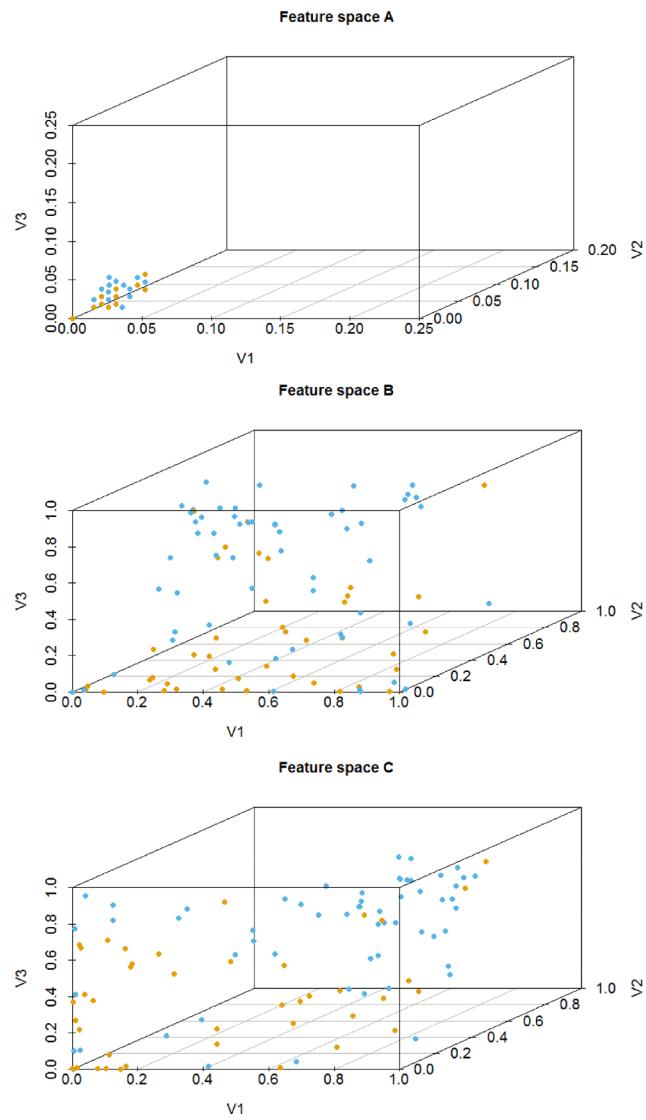


Fig. 6. Visualization of 100 participants in 3 dimensions. (a) original space with some points overlapped, (b) feature space learned by SAE with 20 hidden units, (c) feature space learned by SAE with 30 hidden units. Each dot represents a participant. The color of the dot indicates the outcomes, orange for AD, and blue for NDC, respectively.

features in transformed spaces is not only reduced but also more clearly representing the two outcome groups.

Fig. 7 shows the correlation matrices of features in different spaces constructed. The shaded rectangular tiling represents the correlation value of the corresponding two attributes. It uses a color scale ranging from blue (low correlation value) to red (high correlation value). It indicates that most features in the original space are not conditional independent of each other. The features in 20- and 30-dimensional spaces are approximately uncorrelated. It demonstrates that SAE reduces the dependence of samples' attributes.

3.2. Construction of base classifiers

This section evaluates the performance of the classifiers constructed by multiple classification algorithms on samples of subset1 in three feature spaces. Here are some details of the classifiers. The structure learning method of Bayes network is a hill climbing search for optimal Bayes score. The maximum likelihood estimates method is used for the parameter learning with the obtained structure. The filtered classifier is a combination of the J48 decision tree and the MDL discretization

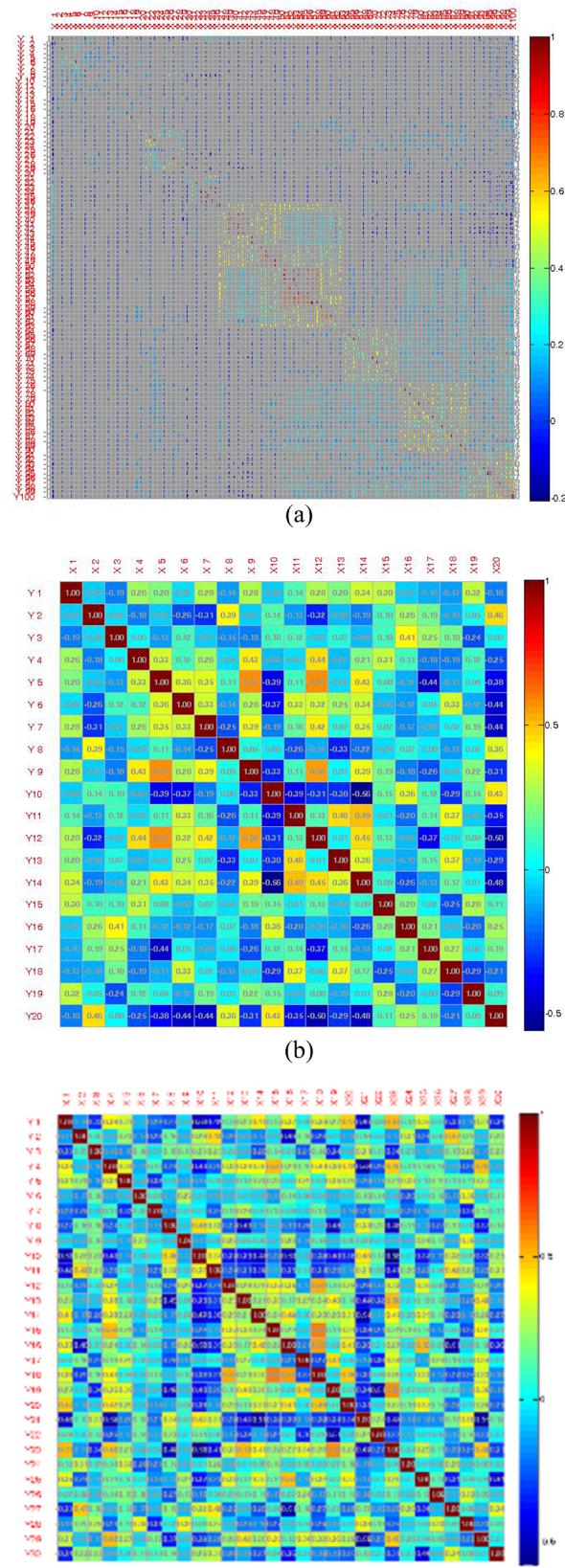


Fig. 7. Correlation matrix of three feature spaces. (a) original space, (b) 20-dimensional space transformed by SAE, (c) 30-dimensional space transformed by SAE.

method [49]. The minimum number of participants in the leaf is set to 2. 3-fold of participants is used for pruning with the confidence factor is 0.25. The rest is used for growing the tree. Hoeffding tree is an incremental anytime decision tree induction algorithm, which splitting criterion is the Gini index. The leaf prediction strategy is set to the majority class. REPTree is a decision tree using information gain and prunes with reduced-error pruning with backfitting. Random subspace consists of multiple REPTree constructed systematically by randomly selecting 50% components of all features. The activation function of Multilayer Perception is a sigmoid function. The number of hidden units is set to 51, 11, and 16 for the models in 3 different feature spaces. The learning rate is set to 0.3. Momentum is 0.2. The others adopt the standard parameter settings.

Table 4 to **Table 7** shows the performance of classifiers in the reduced feature spaces, namely 20- and 30-dimensional spaces learned by SAE, which are comparable with the original feature space. It indicates that our feature learning method not only dramatically reduces the correlation of clinical measures but also retains the useful information. The classifiers with better performance are selected as the base classifiers. At the same time, physicians in different fields can be imitated by these classifiers.

Through these different learning algorithms and feature spaces, the diversity of these base classifiers or physicians has been improved. Here is an example to validate it. **Table 8** shows the classification results of Logistic Regression (LR) and REPTree (RT) in the 20-dimensional feature space. N_{11} and N_{00} are the numbers of participants that are correctly and wrongly recognized by these two classifiers, respectively. N_{10} is the number of participants who were correctly diagnosed by LR but wrongly diagnosed by RT, and N_{01} vice versa. The Q statistics between LR and RT is 0.86, which is smaller than 1. It shows that these two classifiers tend to recognize the same individuals correctly.

$$Q_{LR,RT} = \frac{N_{11}N_{00} - N_{01}N_{10}}{N_{11}N_{00} + N_{01}N_{10}} = \frac{14354175 - 1055716}{14354175 + 1055716} = \frac{13298459}{15409891} \approx 0.86$$

Let X be the number of base classifiers that correctly identify a participant. The variance of X is a measure of diversity based on the distribution of difficulty. **Fig. 8(a)** shows that all classifiers in the group made the correct predictions for around 4500 samples in the test dataset. All base classifiers which are trained by different learning algorithms and feature spaces achieved relatively high performance. Diverse groups of classifiers will have a smaller variance of X . Here, $X=1.1751e+06$. As shown in **Fig. 8(b)**, after using our classifier ranking method in the stacking layer, we observed that the base classifiers No. 3 and 5, have the highest score whose prediction accuracy are concurrently higher. Therefore, DELearning can evaluate classifiers or physicians automatically.

3.3. Stacking by DBN

We formulate each participant as a vector composing of the predictions of these base classifiers. DBN is trained on the training set to ensemble these opinions from base classifiers with a greedy layer-wise unsupervised method in a mini-batch size of 100 cases [50]. Obvious biases and weights are initialized to 0, and random numbers obeyed a zero-mean normal distribution with a standard deviation 0.01. Momentum is set as 0.5. We run 100 epochs with a learning rate of 0.002. Here, we compare different settings of the number of hidden units from

Table 8

The relationship between Logistic Regression and REPTree in classification on 20-dimensional feature space.

	RT correct(1)	RT wrong(0)
LR correct(1)	$N_{11}(7535)$	$N_{10}(1102)$
LR wrong(0)	$N_{01}(958)$	$N_{00}(1905)$

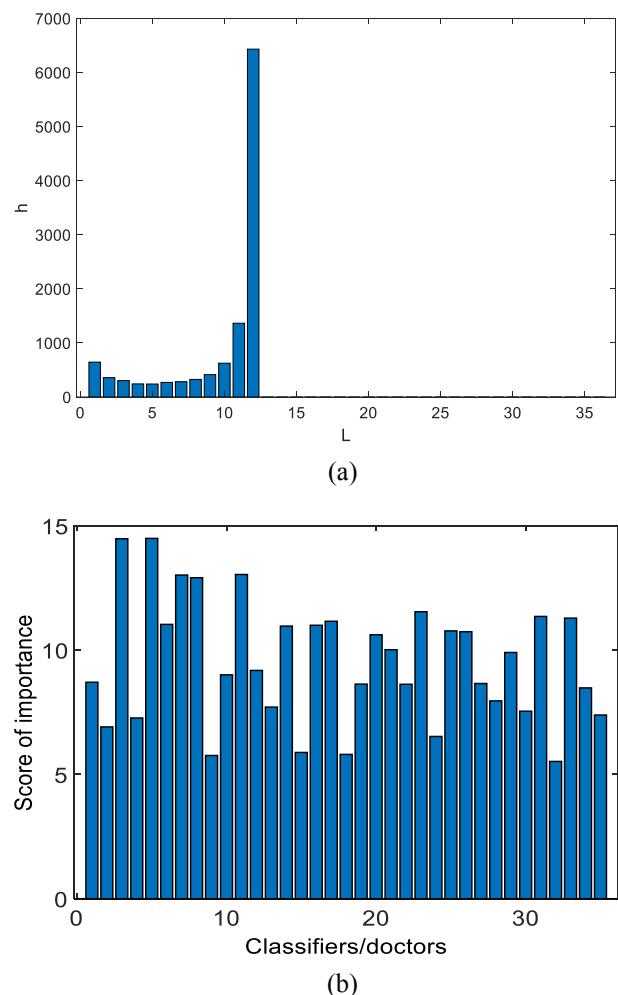


Fig. 8. (a) Patterns of difficulty θ for classifiers group with $L = 35$, $N = 11500$ and $p > 0.7$. The histograms show the number of samples that are correctly diagnosed by classifiers. The x-axis is the number of classifiers. (b) The important score of base classifiers calculated by DELearning. The x-axis indicates the classifier number. The y-axis is the score of the corresponding classifier.

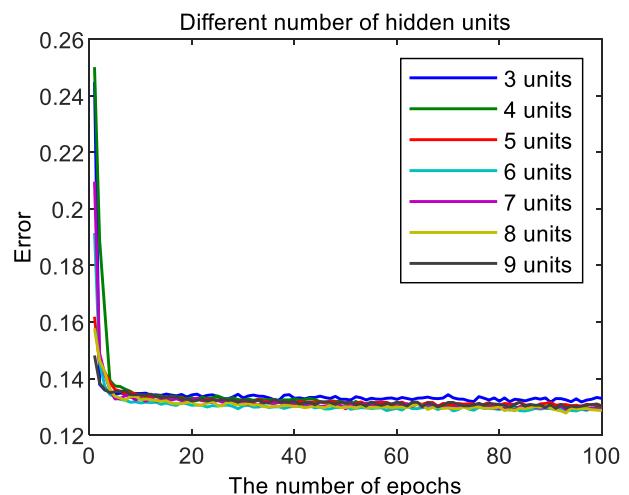


Fig. 9. Errors with different sizes of hidden layers.

3 to 9. Refer to **Fig. 9** for the details. The DBN with 6 hidden units has the lowest error, and so it is selected. The trained DBN is used to initialize artificial neural networks.

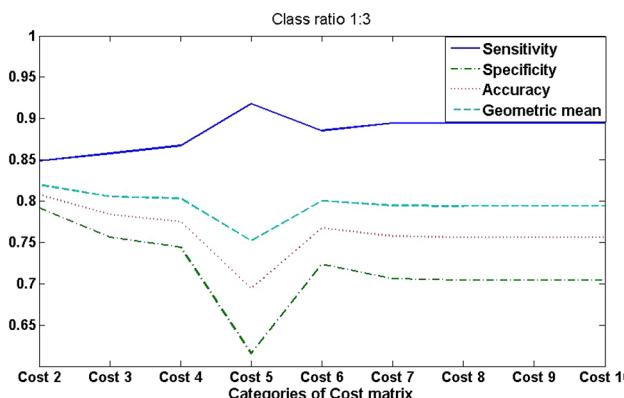


Fig. 10. The performance of NNs with different cost matrixes.

3.4. Optimization for the final decision

We compare 9 cost matrixes with integer values between 2.0 and 10.0. Each matrix is required to have at least one non-diagonal element to be equal to 1. From Fig. 10, we can see that the Geometric mean of cost 2 is highest; the cost matrix we used are shown in Table 9.

Specifically, after all the parameters are determined by training on training set in which the validation set is included in it, we compared DELearning with six ensemble learning methods, including LogitBoost [51], Bagging [52], Random Forest [53], AdaBoostM1 [54], Stacking [55], Vote [56]. As shown in Fig. 11, our method outperforms other ensemble methods in terms of precision, recall, accuracy, and F1-measure, with increases in the recall and accuracy of more than 3% and 4%, respectively. The differences between the performances of DE-Learning and benchmarks are statistically significant, with $P < 0.001$.

Two cost-sensitive learning strategies, including over-sampling and threshold-moving, are adopted in optimizing layer to improve the AD recognition ability of our model by respectively manipulating data and model. By modifying the distribution of the training data, over-sampling technology creates a balanced dataset that provides more AD cases for training NN. By moving the decision threshold of NN toward AD outcome, threshold-moving makes AD cases harder to be misclassified by the NN. The higher recall of our method indicates that more AD cases can be correctly detected. Our method has a low probability of a missed diagnosis of AD whose cost is higher than that of misdiagnosis in the primary care settings. For the application scenario of this paper, high recall is more important than high precision since averaged physicians in primary care settings are interested in screening cases that may be AD. Then, these cases can be advised to go to a superior hospital for more medical resources to confirm the diagnosis. This approach could alleviate the pressure on superior hospitals with more and more demands on the service of AD diagnosis. From another perspective, through combining opinions of multiple primary care physicians simulated by base classifiers, the higher accuracy and recall can be achieved by our method. It could help boost the primary diagnosis of AD. The scarce medical resources can then be well allocated, especially for the areas where diagnostic coverage is low. It could help boost the primary diagnosis of AD, especially for the areas where medical resources are scarce.

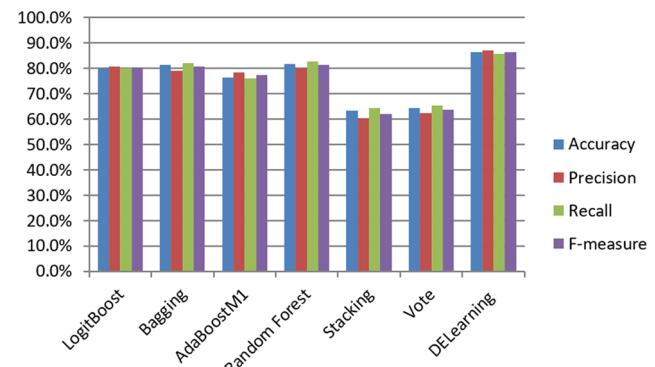


Fig. 11. The performance comparison of DELearning with six representative ensemble learning methods on NACC UDS.

4. Conclusions

The challenge of AD classification leads us to leverage the wisdom of experts and integrate multisource data to come up with better outcome prediction modality that could be used in primary care. This paper proposes DELearning, a three-layer framework, for AD classification that uses the deep learning approach to ensemble at each layer.

Using the clinical data from NACC UDS, we compared the performance of DELearning with six representative ensemble learning methods. The experimental results show that DELearning outperforms the others in terms of AD classification accuracy. It provides a data-driven solution to aid AD primary care, especially where access to AD expertise is limited.

DELearning can also be applied to other scenarios, including medical image tagging, where it may be not feasible or too expensive to obtain objective and reliable labels. DELearning can collect subjective labels from multiple experts or annotators and find meaningful yet hidden labels.

Author contributions section

The authors' contributions were as follows—Ning An and Huitong Ding: designed the study and wrote the paper; Jiaoyun Yang, Huitong Ding, Ning An: performed the analysis; Jiaoyun Yang, Rhoda Au and Ting F. A. Ang: interpreted the results; Rhoda Au, Ting F. A. Ang: edited the manuscript; and all authors: read and approved the final manuscript.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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Table 9
Cost matrix used in DELearning.

	AD	NDC
AD	0	2
NDC	1	0

Sano, PhD), P30 AG008051 (PI Thomas Wisniewski, MD), P30 AG013854 (PI M. Marsel Mesulam, MD), P30 AG008017 (PI Jeffrey Kaye, MD), P30 AG010161 (PI David Bennett, MD), P50 AG047366 (PI Victor Henderson, MD, MS), P30 AG010129 (PI Charles DeCarli, MD), P50 AG016573 (PI Frank LaFerla, PhD), P50 AG005131 (PI James Brewer, MD, PhD), P50 AG023501 (PI Bruce Miller, MD), P30 AG035982 (PI Russell Swerdlow, MD), P30 AG028383 (PI Linda Van Eldik, PhD), P30 AG053760 (PI Henry Paulson, MD, PhD), P30 AG010124 (PI John Trojanowski, MD, PhD), P50 AG005133 (PI Oscar Lopez, MD), P50 AG005142 (PI Helena Chui, MD), P30 AG012300 (PI Roger Rosenberg, MD), P30 AG049638 (PI Suzanne Craft, PhD), P50 AG005136 (PI Thomas Grabowski, MD), P50 AG033514 (PI Sanjay Asthana, MD, FRCP), P50 AG005681 (PI John Morris, MD), P50 AG047270 (PI Stephen Strittmatter, MD, PhD).

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