

Fusing Tabular Features and Deep Learning for Fetal Heart Rate Analysis: A Clinically Interpretable Model for Fetal Compromise Detection

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Abstract— Objective: Cardiotocography (CTG) is commonly used to monitor fetal heart rate (FHR) and assess fetal well-being during labor. However, its effectiveness in reducing adverse outcomes remains limited due to low sensitivity and high false-positive rates. This study aims to develop an interpretable deep learning model that fuses FHR time series with tabular clinical features to improve prediction of fetal compromise (umbilical artery pH < 7.05). **Methods:** We introduce Fusion ResNet, a novel architecture combining residual convolutional networks for FHR signal processing with a parallel neural network for tabular features. The model was trained and internally validated on a private dataset of 9,887 FHR recordings. External validation was performed on the open-access CTU-UHB dataset comprising 552 recordings. Model interpretability was evaluated using Shapley Additive Explanations (SHAP) and Gradient-Weighted Class Activation Mapping (Grad-CAM). **Results:** Fusion ResNet achieved a mean area under the ROC curve (AUC) of 0.77 during internal cross-validation and a state-of-the-art AUC of 0.84 on the CTU-UHB dataset, outperforming existing deep learning approaches. SHAP analysis identified key clinical features contributing to predictions, while Grad-CAM highlighted salient FHR patterns linked to fetal compromise. **Conclusion:** The proposed model enhances predictive accuracy while providing clinically meaningful explanations, enabling more transparent and reliable CTG interpretation. **Significance:** This work demonstrates the potential of interpretable deep learning to improve fetal monitoring by integrating multimodal data, supporting timely and informed decision-making in obstetric care.

Index Terms— Cardiotocography, Deep Learning, Electronic Health Records, Explainability, Fetal Heart Rate

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I. INTRODUCTION

INTRAPARTUM stillbirths account for 45% of stillbirths worldwide [1]. A leading cause of intrapartum stillbirths is fetal asphyxia. It is caused by impaired placental blood gas exchange during labor leading to reduced oxygen supply to fetal tissues followed by acidosis compromising fetal wellbeing [2]. Causes of fetal asphyxia may include maternal hypo-tension, poor placental perfusion, and umbilical cord compressions [2]. The compensatory fetal responses to oxygen deprivation are reflected as abnormal changes in the fetal heart rate (FHR). Clinicians monitor the FHR to detect potential events that may compromise fetal well-being, allowing timely intervention through a cesarean section or instrumental delivery to prevent adverse outcomes.

The most widely used technique for FHR monitoring is cardiotocography (CTG), which simultaneously records the FHR and uterine activity [3]. These signals are visually evaluated based on consensus guidelines for intrapartum fetal monitoring such as the International Federation of Gynecology and Obstetrics guidelines (FIGO) [4]. Therefore, CTG interpretation is subjective and marked by significant intra- and interobserver variability [5]. Despite more than five decades of widespread use since its introduction in the 1960s, CTG has yet to show a significant impact in reducing neonatal mortality or long-term neurological impairment [4], [6]. However, its association with increased cesarean section rates has raised ongoing concerns [4], [6]. Furthermore, in clinical practice, the true positive rate (TPR) for detecting fetal compromise is low, typically ranging from 31% to 48%, with a false positive rate (FPR) between 16% and 21% [7], [8].

Recent research has proposed data-driven systems using machine learning (ML) and deep learning (DL) methods for FHR evaluation [7], [9]–[12] aiming to address the challenges of observer variability, low sensitivity, and high false positive rates associated with visual CTG interpretation. The ML classifiers commonly used for feature-based FHR evaluation are support vector machines (SVM) [8], [9] and logistic regression [13], [14]. Primarily, these ML methods use classical FHR features (e.g.: baseline, variability, accelerations, and decelerations) and/or human-crafted new features using feature selection and

73 feature extraction [12]. Among these new features, decelerative
74 capacity from phase-rectified signal averaging (DC_{PRSA}),
75 median absolute deviation of FHR (MAD_{dtrd}), β_0 parameter
76 representing the FHR baseline, and the Hurst parameter
77 (H) have shown strong classification performance for fetal
78 compromise detection [9], [15]. In contrast, DL methods learn
79 directly from the raw FHR signals and may evaluate novel
80 features that do not have a clear physiological meaning [16].
81 These methods often use feedforward neural networks such
82 as convolutional neural networks (CNNs) [7], [10], [17], and
83 recurrent neural networks such as long short-term memory
84 (LSTM) networks. Existing works have shown that CNNs
85 outperformed LSTMs as well as other ML methods in fetal
86 compromise detection [10], [18], [19]. The main challenges
87 for these DL methods are the limited availability of CTGs for
88 training and interpretability [10], [16]. The current state-of-the-
89 art performance reported on the public CTU-UHB intrapartum
90 CTG dataset is by a multimodal CNN (MCNN) using the raw
91 CTG signals along with quality features calculated based on the
92 percentage of signal loss present in the signal. It was trained
93 on over 35,000 CTGs and achieved an area under the receiver
94 operating characteristic curve (AUC) of 0.81 by evaluating the
95 last 60 minutes of CTG regardless of labor.

96 Prior evidence demonstrates that adverse outcomes are influenced
97 by other clinical risk factors, including meconium-stained
98 fluid, gestational diabetes, hypertension, and fetal growth restriction
99 [14], [16]. Several studies have shown that including
100 such factors, which are typically captured in electronic health
101 records (EHR), alongside FHR features could improve fetal
102 compromise detection [13], [14]. A recent retrospective study
103 combined two FHR features and two clinical risk factors into a
104 computerized CTG system (OxSys 1.5) and showed increased
105 sensitivity for fetal compromise detection and reduced the
106 false-positive rate [7], [11]. Another recent multicohort study
107 investigated the impact of signal loss in CTG signals on perinatal
108 asphyxia and found a strong association and concluded
109 that integrating measures of signal loss into fetal monitoring
110 algorithms may improve decision-making [20].

111 More recent studies have further advanced computerized
112 CTG interpretation through transformer-based and multimodal
113 deep learning architectures. For example, 1D-U-Net-based
114 models that jointly analyze fetal heart rate and uterine activity
115 signals have demonstrated improved accuracy and reliability in
116 detecting abnormal CTG patterns [21]. Similarly, transformer-
117 based frameworks, such as PatchCTG, have demonstrated robust
118 performance in identifying high-risk cases during antepartum
119 monitoring [22]. The integration of large language models
120 into CTG interpretation has also been explored, highlighting the
121 potential of natural language-augmented decision support to enhance
122 interpretability and clinical confidence [23]. Furthermore,
123 DeepCTG® 2.0, a CNN-based model validated across multiple
124 clinical centers, demonstrated strong predictive capability for
125 detecting neonatal acidemia during labor, with AUC values
126 ranging from 0.74 to 0.83. The study also emphasized that
127 incorporating relevant clinical variables could further enhance
128 model performance by accounting for risk factors not evident
129 in CTG signals [24].

130 Despite the existing literature on fetal compromise detection,

131 no study has investigated the integration of these tabular
132 features with DL models that use raw FHR as input and
133 explored their interpretability. This study proposes a novel
134 deep learning approach that builds on a previously established
135 processing workflow and generalizable model to integrate
136 tabular features with raw FHR time series for improved fetal
137 compromise detection, with performance validated across two
138 international CTG cohorts [10]. Furthermore, the model ex-
139 plainability is investigated to understand the models' decision-
140 making process in both a global manner and based on individual
141 case explanations to assist with clinical adoption.

142 The primary contributions of this study are as follows:

- Propose a novel deep learning fusion model to integrate
143 tabular clinical features and classical FHR features with
144 raw time-series FHR signals to enhance fetal compromise
145 detection.
- Assess performance of traditional feature-based methods
146 and deep learning fusion models on both internal and
147 external validation data.
- Integrate two explainability AI techniques, SHAP and
148 Grad-CAM, to improve the clinical interpretability of the
149 model predictions and demonstrate their alignment with
150 clinical knowledge.

II. MATERIALS AND METHOD

A. Data acquisition

154 This work uses retrospective FHR records and electronic
155 health records acquired from two international cohorts: Aus-
156 tralia and the Czech Republic. The first cohort consists of
157 FHR records acquired from laboring women of gestation more
158 than 36 weeks who had singleton deliveries between January
159 2010 and December 2021 at the Mercy Hospital for Women,
160 Heidelberg, Melbourne, Australia. The Mercy Health Human
161 Research Ethics Committee of the hospital approved the data
162 extraction (Approval Number 2020-077). The FHR signal
163 data were extracted from the Philips IntelliSpace Perinatal™
164 information system with technical support from Philips. The
165 maternal, fetal, and neonatal information related to each deliv-
166 ery was extracted from the Birthing Outcomes System (BOS)
167 electronic medical record software. This study only selected
168 the FHR recordings ending within 1 hour of birth and had a
169 cord blood pH evaluation within 40 minutes of birth resulting
170 in 9,887 records. Hereafter, this dataset is referred to as "MHW-
171 pH". For a detailed data selection process, we refer the reader
172 to our prior study [10].

173 The second cohort was acquired between April 2010 and
174 August 2012 at the obstetrics ward of the University Hospital
175 in Brno, Czech Republic. The data extraction was approved by
176 the Institutional Review Board of University Hospital Brno
177 and all women have signed informed consent. It consists of
178 552 FHR records linked with electronic health records
179 including cord pH and clinical features [25]. These records are
180 available for public access in the PhysioNet database repository
181 (<https://physionet.org/content/ctu-uhb-ctgdb/1.0.0/>).
182

183

184 B. Data preprocessing, splitting, and labeling

185 In this study, the last 60 minutes of the FHR signal regardless
186 of the stage of labor were analyzed following prior works [7],
187 [10], [17]. The FHR signal was preprocessed by removing arte-
188 facts and linearly interpolating short signal gaps of less than 15
189 seconds. Signal gaps longer than 15 seconds were considered
190 as zero values for input to further data processing. The 15-
191 second threshold for FHR gap interpolation was selected based
192 on empirical evidence from prior fetal heart rate studies [12],
193 [26]–[28], which demonstrated that interpolating short gaps
194 maintains signal integrity, whereas longer imputations introduce
195 distortion. Then, the FHR signal was smoothed down to 1 Hz to
196 remove redundant beats and improve computational complexity
197 while maintaining performance as determined by prior work
198 [12]. The missing values in the tabular features were minimal
199 (<0.4%) and were inputted using the mean of the respective
200 feature. The UC signals were not used in the study due to
201 their poor quality, and no improvement in fetal compromise
202 detection performance was observed in a previous study [12].
203 All FHR recordings of both datasets were included irrespective
204 of their signal loss to reflect real clinical behavior.

205 The MHW-pH data was split into training and validation
206 datasets using 5-fold cross-validation. The CTU-UHB dataset
207 was used as an external testing dataset. The MinMax scaler
208 normalization was applied for the FHR time series signals on
209 both datasets. The tabular features were standardized with a
210 zero mean and unit variance.

211 As the outcome-defining criterion, this study uses the arterial
212 cord blood pH. It measures the acidity of fetal blood just after
213 birth which is used as an objective biochemical indicator for
214 identifying potentially compromised babies. This criterion has
215 been widely used by existing studies for computerized fetal
216 compromise detection to label their data. Predominantly, births
217 with $pH < 7.05$ were labeled as the compromised class [7],
218 [10], [12], [19]. This study uses the same threshold to label
219 the datasets into Normal and Compromised classes following
220 prior work for fair comparisons.

221 C. Tabular features

222 This study analyzed twelve tabular features composed of
223 electronic health records (EHR), enhanced FHR features used
224 in classical machine learning, and features related to signal qual-
225 ity. Specifically, six EHR features—Parity, Gestation, Maternal
226 Age, Diabetes, Hypertension, and Meconium were selected as
227 they were available in both cohorts. The first three features
228 were used as real values and the remaining three as boolean
229 values. In practice, these features are readily available for
230 clinicians as clinical data for decision-making before delivery.

231 As FHR features, four enhanced FIGO features—median ab-
232 solute deviation of FHR after baseline subtraction (MAD_{dtra})
233 [9] quantifying the average depth of FHR, the intercept of
234 the linear regression model for the evolution of baseline
235 along time (β_0) [9], Hurst parameter (H) [9] quantifying
236 the variability of FHR and the decelerative capacity of FHR
237 calculated from the phase rectified signal averaging method
238 (DC_{PRSA}) [15] quantifying the average downward movement
239 of FHR. These four FHR features are identified as top features

240 in prior works for automated fetal compromised detection
241 using classical machine learning methods [9], [11]. This study
242 utilized the original implementation available in their respective
243 studies to calculate these features. The FHR features were
244 calculated on the last 60 minutes of the 4 Hz FHR signal. To
245 include the impact of signal loss inherent to FHR monitoring
246 methodologies, this study used two features related to signal
247 quality—the ratio of zeros in the FHR signal (SigLoss) and
248 the mode of FHR acquisition (AqMode). The AqMode feature
249 is used as a categorical variable coded with 1, 2, and 3
250 representing Doppler ultrasound-based FHR acquisition, direct
251 fetal electrocardiogram using fetal scalp clip, and use of both
252 respectively.

253 D. Feature ranking and machine learning approach

254 The tabular features were first ranked using the minimum
255 Redundancy Maximum Relevance (mRMR) feature selection
256 algorithm as shown in Fig. 1a. The mRMR algorithm selects
257 the most relevant features to the class labels while minimizing
258 the redundancy among the selected features [29]. All the ranked
259 tabular features were analyzed using classical machine learning
260 methods in the literature for fetal compromise detection. Specif-
261 ically, this study compared the area under the receiver operating
262 characteristic curve (AUC) performance for classifying fetal
263 compromise using two support vector machine (SVM) methods
264 already used for fetal compromise detection—classical linear
265 SVM [30], and Sparse linear SVM with ℓ_1 -norm as penalty
266 and squared Hinge loss function (instead of standard ℓ_2 -norm
267 as penalty and Hinge loss) [9].

268 Each SVM method was evaluated in two experiments as
269 shown in Fig. 1b. First, these features were evaluated using a
270 stratified 5-fold cross-validation (CV) on the MHW-pH dataset.
271 Then, the trained model on each fold was externally tested
272 on the CTU-UHB dataset. During training, the class weights
273 were adjusted inversely proportional to class frequencies in
274 the input data to tackle the class imbalance. In all analyses,
275 the regularization parameter C, which controls the trade-off
276 between misclassification rate and data sparsity in SVM
277 classifiers was optimized using a grid search with a 5-fold
278 CV.

279 To compute the performance, each feature was first used in a
280 univariate evaluation. Then the ranked features were iteratively
281 evaluated with the SVM methods by adding one feature at a
282 time to perform a multivariate analysis.

283 E. Fusion of tabular features and deep learning

284 This study proposes a novel deep learning model for fetal
285 compromise detection that fuses tabular features with time
286 series FHR, building upon the previously established ResNet-
287 based architecture and optimum processing workflow [10]. An
288 overview of the Fusion ResNet model architecture with two
289 inputs (FHR time series and tabular features) is shown in
290 Fig. 2a. The top five ranked tabular features from the mRMR
291 algorithm evaluated on the MHW-pH dataset were selected for
292 the deep learning approach.

293 The input to the ResNet branch is the 60-minute FHR
294 time series (3600 values sampled at 1Hz). The ResNet model

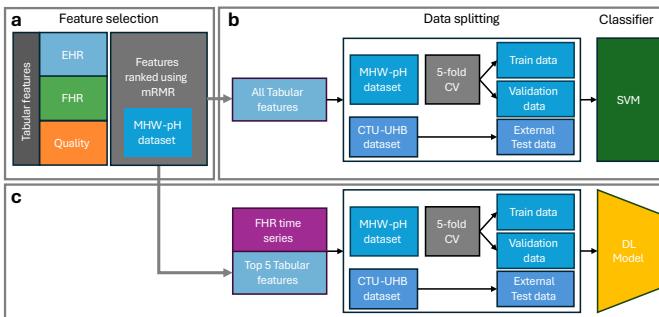


Fig. 1. Panel (a) shows the feature ranking of EHR ($n=6$), FHR ($n=4$), and Quality ($n=2$) features using the minimum redundancy maximum relevance (mRMR) feature selection algorithm. Panel (b) illustrates the data splitting and performance evaluation of all ranked tabular features with the SVM classifier (Classical SVM and Sparse SVM). Panel (c) illustrates the use of the top five tabular features ranked by using the mRMR method on the MHW-pH training dataset, along with the FHR time-series signal for deep learning evaluation. In both evaluations, the MHW-pH dataset was used for the 5-fold CV, while CTU-UHB was used as the external testing data.

consists of three residually connected 1D convolutional blocks. The output of the last convolution block is passed through a global average pooling layer (GAP) that averages the temporal dimension to a single value resulting in a feature vector equal to the number of filters of the last convolutional layer (1×128 in this case). More details of the ReNet model architecture are given in our prior work [10]. The tabular features are processed through a second branch comprising two fully connected (FC) hidden layers with output dimensions of 10 and 128, respectively. A dropout layer is included between the FC layers to reduce the risk of overfitting. The first FC layer uses a rectified linear unit (ReLU) activation function, while the second employs a sigmoid activation function to constrain the output range. The feature vectors from both branches are combined via a fusion operator and subsequently passed through a final output layer with a sigmoid activation function to generate the predicted class probabilities. Three fusion operators were evaluated: element-wise multiplication, addition, and concatenation.

In training and evaluating this proposed Fusion ResNet model, we used a stratified 5-fold CV on the MHW-pH dataset and used CTU-UHB as the external testing dataset as shown in Fig. 1c. The cases with pH that belong in the range, $pH \geq 7.05$ and $pH < 7.15$ (intermediate cases), were removed from the training data to minimize potential errors in the labels as it is not well established in the literature whether this group consists of compromised events or not [7], [10], [12]. However, the intermediate cases were not removed from the testing datasets as they are present in reality. During the training process, class weights based on inverse class frequency were used to tackle the class imbalance. This ensured heavy penalization for misclassifying minority cases during training. The binary cross entropy was used as the loss function and Adam as the optimizer. All models were trained for a maximum of 400 epochs with a batch size of 16 and an initial learning rate of 0.0001. Early stopping based on validation loss was used to dynamically stop the training.

This study also investigated the use of a pre-trained ResNet

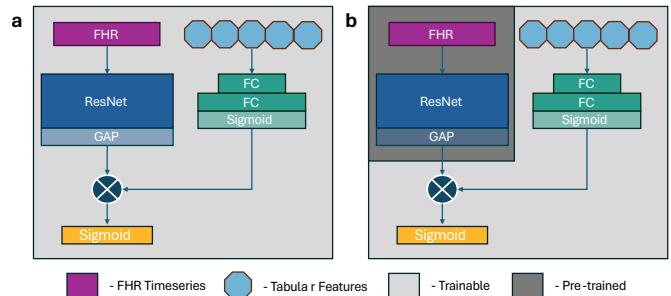


Fig. 2. Fusion ResNet model architecture with two branches, where time series FHR uses the existing ResNet model and tabular features use a dense model in a separate branch. Outputs from both branches are fused via a fusion operator and passed through the final sigmoid layer. Three fusion operators were evaluated: element-wise multiplication, addition, and concatenation. (a) and (b) shows the trainable regions for the trainable model and the pre-trained model, respectively.

branch compared to keeping it trainable during the training process (Fig. 2b). Both trainable and pre-trained deep learning models were independently trained and evaluated by progressively adding tabular features to the model, one at a time, according to their feature importance ranking. The performance of only using the FHR time series branch was also evaluated. As performance metrics, the true positive rate (TPR) at 5%, 10%, 15%, and 20% false positive rate (FPR) and AUC were calculated. The mean and standard deviation of these performance metrics for 5-fold CV on MHW-pH and external test on CTU-UHB for each experiment were reported. The best-performing model was selected based on the 5-fold CV performance on the MHW-pH dataset. All experiments were carried out on an Intel® Xeon® Gold 6326 CPU at 2.90 GHz with an Nvidia A100 GPU and 16 GB of RAM. The models were implemented using the TensorFlow 2.0 framework.

F. Model interpretability

To explain the model predictions of the proposed Fusion ResNet model, this study used Grad-CAM (Gradient weighted Class Activation Mapping) [31] and SHAP (Shapely Additive exPlanations) [32] methods widely used for explainable artificial intelligence. Both methods focus on calculating feature attribution scores assigned to each input of the model to quantify their significance to the prediction made by the model.

The Grad-CAM is used in this study to visualize the regions of the FHR time series that contribute to the model prediction. It uses the channel-wise mean of the gradient information flowing into the last convolutional layer of the ResNet model as weights to calculate a weighted sum of the feature maps in the last convolutional layer. This is then passed through a ReLU function to focus on the positive contributions producing a coarse localization map that highlights the important regions of FHR time series influencing the model prediction.

The SHAP values are used in this study to visualize the contributions of tabular features and FHR time series as a whole for the model prediction. To compute the SHAP values, we use SHAP DeepExplainer [32] from the SHAP package. The SHAP values ensure a fair distribution of importance among the input features based on their contributions to the

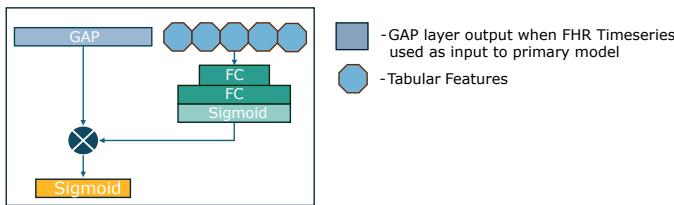


Fig. 3. Secondary fused deep learning model used with SHAP DeepExplainer. All corresponding layer weights were replicated from the trained primary model.

model output. Applying SHAP directly to the FHR time series would produce 3600 SHAP values which will be hard to interpret and aggregate to compare with the SHAP values from tabular features. Therefore, as illustrated in Fig. 3, we created a secondary model with the GAP layer (128 values) from the primary model as input for the FHR time series branch. All layers of the secondary model were replicated with the corresponding layer weights from the primary model. The 128 GAP values are a compressed representation of the time series, and computing SHAP on these values enables more meaningful and computationally efficient insights. To generate a single SHAP value representing the FHR time series, we aggregated the 128 SHAP values from the GAP layer using summation. The MHW-pH data was used as the background data for the SHAP DeepExplainer and was tested with the CTU-UHB dataset.

G. Statistical testing

The Mann-Whitney U test was used to test the statistical significance of the tabular features for the Normal and Compromised groups. The same test was used to test the significant differences between the AUC performance of the Fusion ResNet model on CTU-UHB for all tabular feature pairs including the FHR time series. The Pearson correlation testing was used to compute the significance of the correlation among the tabular features.

III. RESULTS

A. Data distribution and correlation

This study evaluated automated fetal compromise detection using the last 60 minutes of the FHR time series in labor from two international cohorts from Australia (MHW-pH, n=9,887) and the Czech Republic (CTU-UHB, n=552). The participant characteristics of the two cohorts are shown in Table I. Cord pH measurements were used as the outcome criterion to divide the data into Compromised ($pH < 7.05$) and Normal classes ($pH \geq 7.05$). This resulted in 40 (7.2%) and 111 (1.1%) cases for the compromised class for CTU-UHB and MHW-pH datasets, respectively.

In addition to the FHR time series, twelve tabular features including six electronic health record features, four enhanced FHR features, and two quality features were included in the analysis. The distributions of twelve features for the two classes in both datasets are shown in Fig. 4a. A significant difference in the parity, MAD_{dtrd} (median absolute deviation of the detrended FHR), DC_{PRSA} (decelerative capacity of FHR), and

SigLoss (ratio of signal loss in FHR) features was observed in the Normal and Compromised classes in both datasets. Additionally, maternal age showed a significant difference in the two classes for the MHW-pH dataset, while β_0 (intercept of the FHR baseline evolution model) was significant for the CTU-UHB dataset. Furthermore, to examine the relationship among the selected features in each dataset, the Pearson correlation was computed and shown as a heatmap in Fig. 4b.

B. Univariate and multivariate feature analysis using classical machine learning

The predictive capability of each tabular feature was individually evaluated using two support vector machine (SVM) models to determine their effectiveness in fetal compromise detection. The AUC performances on the univariate and multivariate feature evaluation using SVM models on 5-fold CV on the MHW-pH dataset and external testing on the CTU-UHB dataset are shown in Fig. 5. The rank of the features for multivariate analysis was determined by the minimum redundancy maximum relevance (mRMR) method on the MHW-pH dataset.

In the univariate analysis using a 5-fold CV on the MHW-pH dataset, the MAD_{dtrd} feature showed the best performance (AUC of 0.66) closely followed by SigLoss (AUC=0.60), DC_{PRSA} (AUC=0.59), and Parity (AUC=0.59) on the Sparse SVM model. Similarly, the MAD_{dtrd} feature achieved the best performance (AUC=0.76) when externally tested on CTU-UHB followed by features SigLoss (AUC=0.71) and DC_{PRSA} (AUC=0.66) using the same Sparse SVM model. In both 5-fold CV and external testing, the Sparse SVM model showed superior performance compared to the Classical SVM model in the majority of the features.

In the multivariate analysis using a 5-fold CV on the MHW-pH dataset, the AUC performance on both SVM models showed an upward trend initially for the first three features (β_0 , Parity, and MAD_{dtrd}), then when more features were added Sparse SVM performance remained marginally stable while Classical SVM performance showed a slight reduction in performance. Both models showed the best AUC performance of 0.69 with the first three features. In contrast, the external test on CTU-UHB showed an initial drop in the performance of both SVM models when the Parity feature was combined with β_0 and then increased sharply with the addition of the MAD_{dtrd} feature and remained relatively stable beyond three features. The AUC performances of the first three features when tested externally on CTU-UHB were 0.75 and 0.74 for Sparse SVM and Classical SVM, respectively.

C. Fusing FHR time series with tabular features using deep learning

The top five ranked features based on the MHW-pH dataset were used to integrate with the time-series FHR data using a deep learning approach to evaluate their performance in fetal compromise detection. The proposed fusion deep learning model (Fusion ResNet) was trained and evaluated in two ways — first with the time series FHR branch as trainable and second with the time series FHR branch as pre-trained. The 5-fold CV performance on the MHW-pH dataset and the external test

TABLE I
PARTICIPANT CHARACTERISTICS OF THE CZECH REPUBLIC AND AUSTRALIAN COHORTS.
STD = STANDARD DEVIATION, IQR = INTERQUARTILE RANGE.

Characteristics	CTU-UHB (n=552)				MHW-pH (n=9887)			
	Mean (STD)	Median(IQR)	Min	Max	Mean(STD)	Median(IQR)	Min	Max
Gestation (weeks)	40(1.13)	40(39-41)	37	43	39.45(1.25)	39.5(38.5-40.3)	36.10	43.10
Maternal Age (years)	29.67(4.54)	30(27-33)	18	46	31.95(4.48)	32(29.05-35)	18	58.1
pH	7.23(0.11)	7.25(7.17-7.3)	6.85	7.47	7.25(0.08)	7.26(7.2-7.3)	6.00	7.52
	n(%)				n(%)			
Parity	0: 376(68.1) 1: 140(25.4) 2: 29(5.2) ≥3: 7(1.3)				0: 6491(65.7) 1: 2460(24.9) 2: 697(7.0) ≥3: 239(2.4)			
Diabetes	37(6.7)				1333(13.5)			
Hypertension	44(8.0)				276(2.8)			
Meconium	64(11.6)				1832(18.5)			

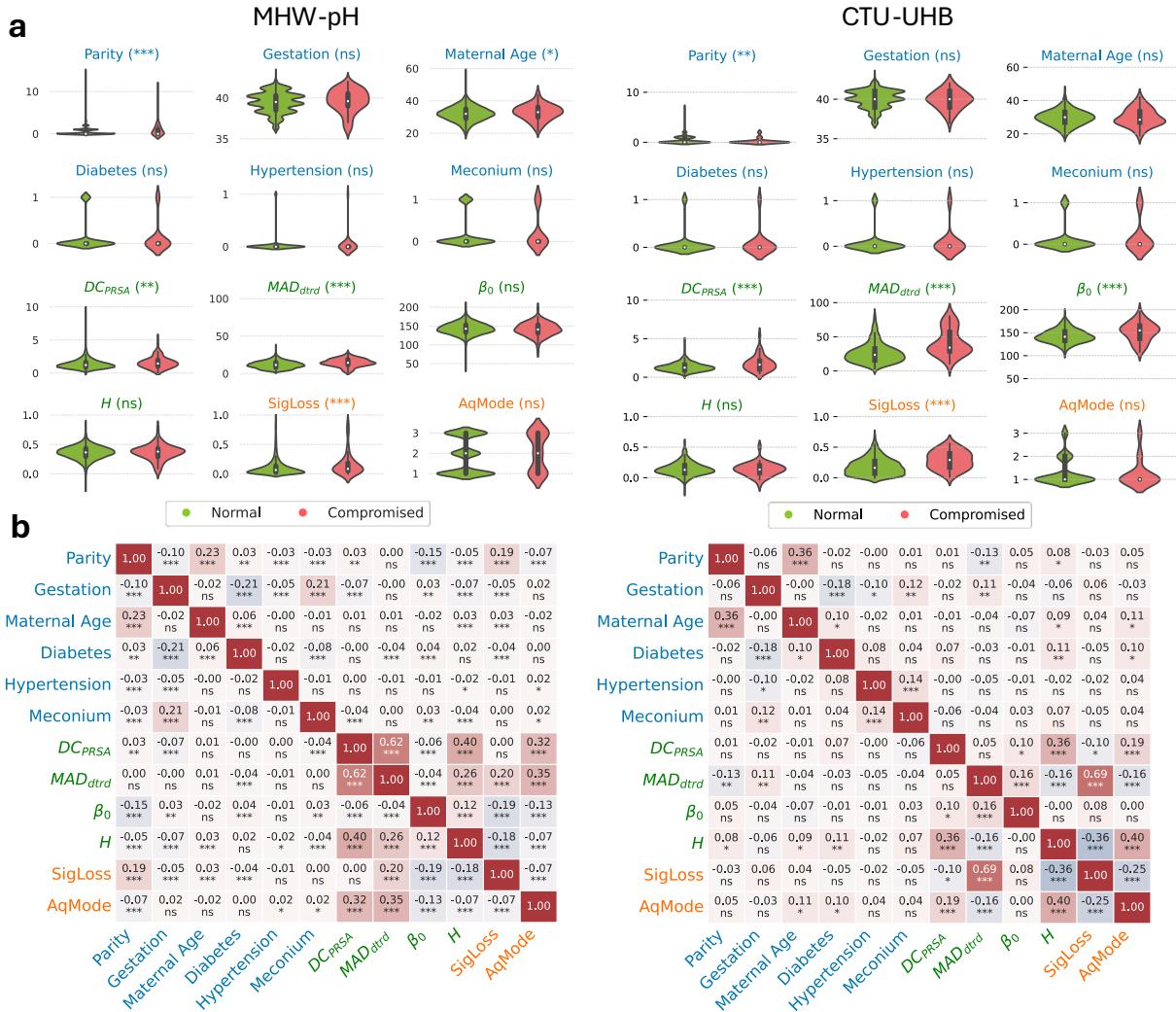


Fig. 4. Top row (a) Violin plots illustrate the distribution of features for the two classes: Compromised ($\text{pH} < 7.05$) and Normal, in two international cohorts. Bottom row (b) Heatmap of Pearson correlation among tabular features consisting of Electronic Health Records (EHR) in blue, enhanced FHR features in green, and Quality features in orange. Statistical significance is indicated by asterisk: ns ($p \geq 0.05$), * ($p < 0.05$), ** ($p < 0.01$), and *** ($p < 0.001$).

471 performance on CTU-UHB for the trainable and pre-trained
472 models are given in Table II and Table III, respectively.

473 As observed in Table II, the 5-fold CV and external test

474 results demonstrated that combining tabular features with the
475 FHR time series, using the Fusion ResNet model with a
476 trainable FHR branch, outperformed the model that relied

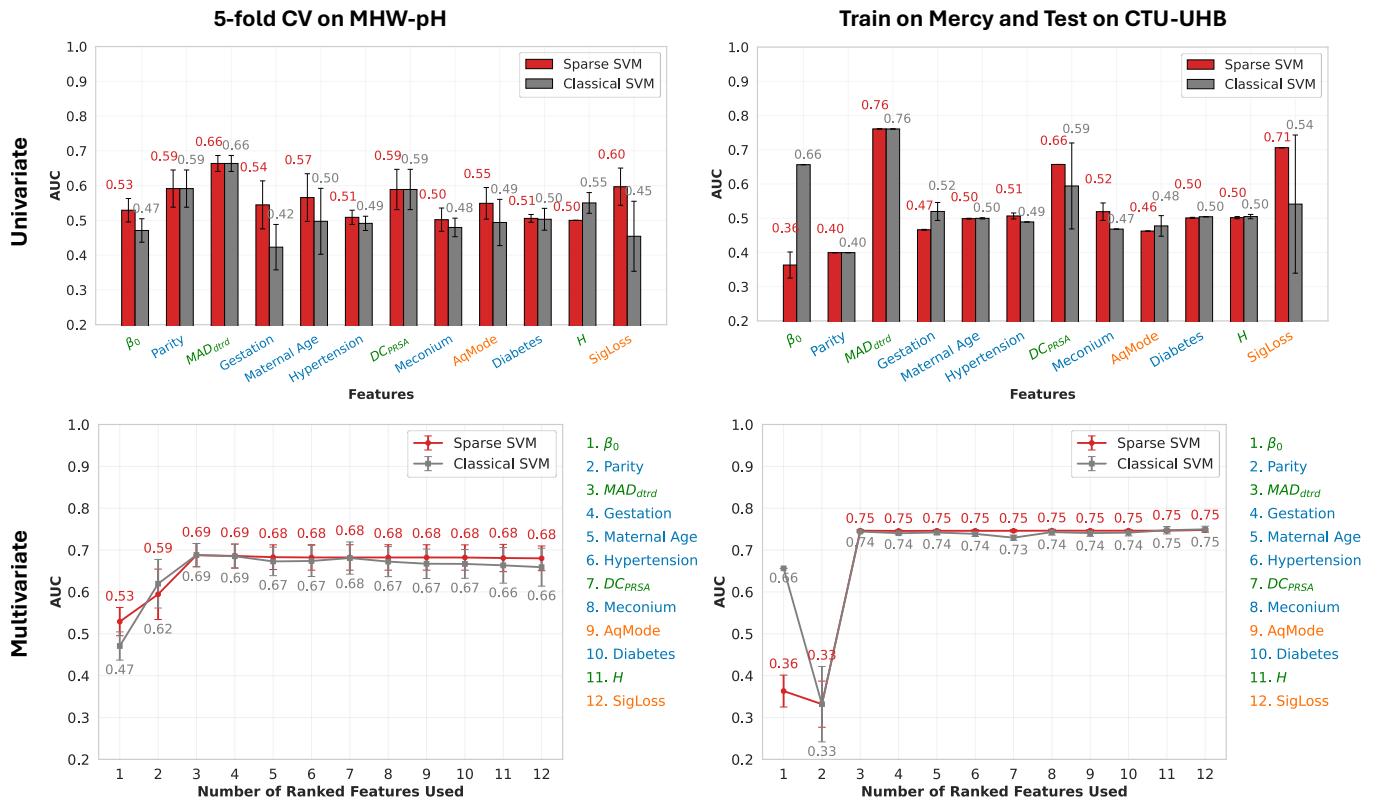


Fig. 5. Univariate and multivariate mean AUC performance of the twelve tabular features evaluated with two types of SVM models using 5-fold cross-validation on the MHW-pH dataset (left column) and when trained on MHW-pH and tested on CTU-UHB (right column). The features were ranked using the minimum redundancy maximum relevance (mRMR) method on the MHW-pH dataset for multivariate evaluation. The same feature order was used for univariate illustrations.

TABLE II
PERFORMANCE OF THE DEEP LEARNING MODELS WITH TRAINABLE FHR BRANCH GIVEN AS MEAN \pm STANDARD DEVIATION. 5-FOLD CV ON MHW-PH AND EACH FOLD MODEL EXTERNALLY TESTED ON CTU-UHB. FINAL MODEL SELECTED BASED ON 5-FOLD CV PERFORMANCE HIGHLIGHTED IN BOLD. FHR = FHR TIME SERIES.

Features	5-fold CV (MHW-pH)				AUC	External Test (CTU-UHB)				AUC		
	TPR (%)					At 5% FPR	At 10% FPR	At 15% FPR	At 20% FPR			
	At 5% FPR	At 10% FPR	At 15% FPR	At 20% FPR								
FHR	26 \pm 8	40 \pm 7	47 \pm 7	50 \pm 8	0.73 \pm 0.04	33 \pm 5	43 \pm 6	54 \pm 4	62 \pm 0	0.80 \pm 0.02		
FHR + β_0	26 \pm 9	39 \pm 7	46 \pm 6	50 \pm 6	0.72 \pm 0.02	43 \pm 4	50 \pm 6	57 \pm 6	65 \pm 5	0.82 \pm 0.04		
FHR + β_0 + Parity	27 \pm 6	41 \pm 9	47 \pm 7	54 \pm 9	0.76 \pm 0.04	33 \pm 6	44 \pm 4	51 \pm 2	61 \pm 2	0.79 \pm 0.02		
FHR + β_0 + Parity + MAD_{dtrd}	26 \pm 7	41 \pm 7	50 \pm 5	60 \pm 5	0.76 \pm 0.04	48 \pm 10	64 \pm 4	70 \pm 4	74 \pm 2	0.85 \pm 0.02		
FHR + β_0 + Parity + MAD_{dtrd} + Gestation	28 \pm 6	40 \pm 6	50 \pm 7	55 \pm 7	0.77 \pm 0.03	45 \pm 3	59 \pm 8	67 \pm 5	72 \pm 4	0.84 \pm 0.02		
FHR + β_0 + Parity + MAD_{dtrd} + Gestation + Maternal Age	22 \pm 6	41 \pm 7	50 \pm 6	56 \pm 5	0.75 \pm 0.03	48 \pm 6	62 \pm 6	70 \pm 6	74 \pm 4	0.85 \pm 0.02		

477 solely on FHR time series data across most tabular feature
 478 combinations. Furthermore, all deep learning models outperformed
 479 the classical machine learning model performance in
 480 5-fold CV on MHW-pH and external CTU-UHB evaluations.
 481 The mean AUC 5-fold CV and external test performance
 482 of the Fusion ResNet model with only FHR time series as
 483 input (without fusing tabular features) were 0.73 and 0.80
 484 respectively. The 5-fold CV performance increased when more
 485 tabular features were added to the model until the fourth feature
 486 and marginally dropped when the Maternal age feature was
 487 added. External evaluation on the CTU-UHB dataset showed

an increase in AUC performance with the addition of the β_0
 488 feature. However, a notable drop in performance occurred when
 489 the Parity feature was included. The subsequent addition of
 490 the next three features resulted in relatively stable AUC values,
 491 with no significant differences among them, but they were
 492 statistically significant compared to the model using only the
 493 FHR time series and model with only β_0 and Parity tabular
 494 features, as illustrated in Fig. 6.
 495

The highest mean 5-fold CV performance (AUC=0.77) as
 496 shown in Table II was achieved by the model that fused the
 497 FHR time series data with the top four tabular features (β_0 ,
 498

TABLE III

PERFORMANCE OF THE DEEP LEARNING MODELS WITH PRE-TRAINED FHR BRANCH GIVEN AS MEAN \pm STANDARD DEVIATION. 5-FOLD CV ON MHW-PH AND EACH FOLD MODEL EXTERNALLY TESTED ON CTU-UHB. FHR = FHR TIME SERIES

Features	5-fold CV (MHW-pH)				AUC	External Test (CTU-UHB)				AUC	
	TPR (%)					At 5% FPR	At 10% FPR	At 15% FPR	At 20% FPR		
	At 5% FPR	At 10% FPR	At 15% FPR	At 20% FPR		At 5% FPR	At 10% FPR	At 15% FPR	At 20% FPR		
FHR	26 \pm 8	40 \pm 7	47 \pm 7	50 \pm 8	0.73 \pm 0.04	33 \pm 5	43 \pm 6	54 \pm 4	62 \pm 0	0.80 \pm 0.02	
FHR + β_0	22 \pm 5	36 \pm 4	43 \pm 3	50 \pm 3	0.73 \pm 0.04	33 \pm 3	44 \pm 5	54 \pm 4	64 \pm 4	0.81 \pm 0.01	
FHR + β_0 + Parity	23 \pm 6	38 \pm 8	45 \pm 4	51 \pm 6	0.74 \pm 0.03	29 \pm 4	42 \pm 8	56 \pm 7	64 \pm 7	0.79 \pm 0.04	
FHR + β_0 + Parity + MAD_{dtrd}	22 \pm 7	35 \pm 6	47 \pm 2	55 \pm 3	0.75 \pm 0.03	35 \pm 6	51 \pm 7	60 \pm 7	68 \pm 6	0.81 \pm 0.05	
FHR + β_0 + Parity + MAD_{dtrd} + Gestation	24 \pm 10	37 \pm 5	49 \pm 4	56 \pm 4	0.74 \pm 0.03	34 \pm 4	49 \pm 10	58 \pm 8	66 \pm 9	0.79 \pm 0.08	
FHR + β_0 + Parity + MAD_{dtrd} + Gestation + Maternal Age	24 \pm 9	37 \pm 4	48 \pm 6	54 \pm 6	0.73 \pm 0.04	39 \pm 6	54 \pm 6	61 \pm 7	69 \pm 1	0.83 \pm 0.01	

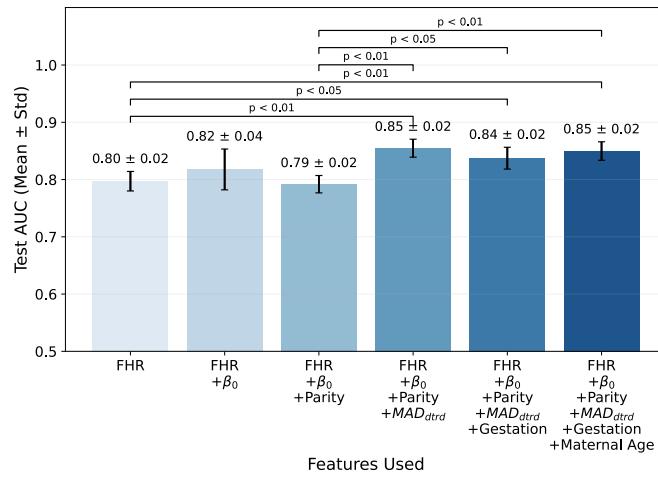


Fig. 6. The comparison of AUC performance in using the Fusion ResNet model with only FHR time series, and the Fusion ResNet model with a trainable FHR branch and a combination of tabular features, tested on the CTU-UHB dataset. A p-value < 0.05 is considered statistically significant. FHR = FHR time series.

Parity, MAD_{dtrd} , and Gestation). The corresponding mean AUC performance on the test CTU-UHB dataset was 0.84 (67–72% TPR at 15–20% FPR). Furthermore, the performance of using a trainable FHR branch, as shown in Table II, achieved superior performance compared to using a pre-trained FHR branch, as shown in Table III, across all evaluated feature combinations.

D. Comparison of Fusion Operators

A comparison study was performed to evaluate the impact of different fusion operators on model performance while keeping all other architectural and training components identical. Three fusion mechanisms were compared: (1) element-wise multiplication, (2) addition, and (3) concatenation. For all variants, the FHR and EHR branches each produced 128-dimensional latent representations before fusion, and the same learning schedules and regularization parameters were applied to ensure a fair comparison.

The results presented in Table IV show that element-wise multiplication achieved the highest internal validation AUC (0.77) and strong external performance (AUC = 0.84) on the

CTU-UHB dataset. The addition and concatenation operators produced comparable but slightly lower internal validation AUCs; however, the concatenation approach achieved superior AUC on the CTU-UHB external validation dataset, at the cost of a slight increase in parameter count.

E. Explaining deep learning model predictions

This study computed SHAP values of the inputs to the Fusion ResNet model to investigate their contribution to the model output. The SHAP values indicate the amount of impact of individual features on the model output. The SHAP beeswarm plot shown in Fig. 7 demonstrates the FHR time series data is the most dominant global feature influencing the model predictions on the CTU-UHB external testing dataset. The MAD_{dtrd} was the next most influential feature, followed by β_0 , Maternal age, and Parity. The Gestation feature is the least influential.

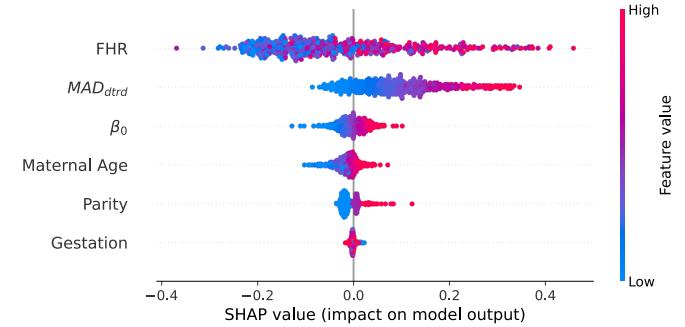


Fig. 7. Beeswarm summary plot illustrating the distribution of SHAP values of tabular features computed for the CTU-UHB dataset indicating the global impact of each feature on the model output.

The positive SHAP values of FHR were generally observed to be associated with high FHR latent space values (3600 FHR values were compressed into a latent space of 128 values and summed to generate a single value, see Method section) while negative SHAP FHR values were observed to be associated with low FHR latent space values. Additionally, high feature values of the MAD_{dtrd} , β_0 , Maternal age, and Parity features showed a clear trend of raising the likelihood of the model prediction towards classification of fetal compromise.

TABLE IV
COMPARISON OF THE SELECTED MODEL PERFORMANCE WITH DIFFERENT FUSION OPERATORS.

Fusion Operator	AUC (MHW-pH, CV)	%TPR at 15% FPR (MHW-pH, CV)	AUC (CTU-UHB)	%TPR at 15% FPR (CTU-UHB)	Params (K)
Multiplication	0.77 ± 0.03	50 ± 7	0.84 ± 0.02	67 ± 5	505.5
Addition	0.74 ± 0.04	47 ± 7	0.79 ± 0.08	57 ± 15	505.5
Concatenation	0.75 ± 0.02	53 ± 2	0.85 ± 0.01	70 ± 4	505.7

544 In addition to SHAP, this study also utilized the gradient
 545 weighted class activation mapping (Grad-CAM) to investigate
 546 the FHR time series regions that strongly impact the model
 547 output. The Grad-CAMs along with the SHAP local bar plots
 548 of four random cases of the CTU-UHB dataset reflecting
 549 true positive, false positive, false negative, and true negative
 550 predictions of the Fusion ResNet model fused with the top five
 551 features are shown in Fig. 8.

552 As illustrated, the true positive case shows that the most
 553 impactful feature for its prediction was the FHR time series
 554 and the Grad-CAM shows strong activation in a deceleration
 555 region of FHR. Higher values of MAD_{dtrd} , β_0 , and maternal
 556 age, reflected by positive SHAP values, contributed positively
 557 to the likelihood of predicting fetal compromise, whereas
 558 being nulliparous, indicated by a negative SHAP value, was
 559 associated with a lower likelihood of being classified as a
 560 compromised case. In the true negative case, the FHR is still
 561 the dominant feature negatively affecting the model prediction,
 562 thus reducing the likelihood of fetal compromise. The Grad-
 563 CAM also aligns with FHR SHAP values as no activated
 564 region corresponding to fetal compromise was observed. Low
 565 MAD_{dtrd} values and moderate β_0 showed negative SHAP
 566 values, reducing the likelihood of fetal compromise. However,
 567 high Gestation showed a negative SHAP value impacting the
 568 model output negatively.

569 For the false positive case, the main contributor to the
 570 higher likelihood of fetal compromise was FHR and Grad-
 571 CAM showed the decelerative regions of FHR impacted the
 572 model strongly. The slightly higher MAD_{dtrd} and slightly
 573 higher β_0 also contributed positively, whereas nulliparous and
 574 low maternal age slightly impacted the model output negatively.
 575 In the false negative case, since no activating regions of FHR
 576 were identified by the model and visualized through Grad-
 577 CAM, the SHAP values for FHR were negative, minimizing the
 578 likelihood of fetal compromise. Nulliparous and low maternal
 579 age further help to minimize the likelihood of fetal compromise.
 580 Although slightly higher MAD_{dtrd} and β_0 positively impacted
 581 the model, they were not strong enough to counter the effect
 582 of FHR. Additional Grad-CAMs and SHAP bar plots for cases
 583 with extreme tabular features are shown in the supplementary
 584 materials.

IV. DISCUSSION

586 Electronic health record features that capture personalized
 587 clinical context along with human-crafted FHR features and
 588 signal quality measures have been shown to be predictive of
 589 fetal compromise in previous studies. However, these features
 590 have not been comprehensively fused with a deep learning

591 based FHR model to assess their combined predictive potential.
 592 This work presents an integrated model that achieves state-
 593 of-the-art performance in fetal compromise detection while
 594 enhancing interpretability, marking a significant step toward
 595 clinically applicable and explainable computer-assisted CTG
 596 analysis.

597 This study first investigated twelve tabular features composed
 598 of extracted FHR features, EHR features, and signal quality
 599 features, ranked using the mRMR feature selection algorithm,
 600 for fetal compromise detection using two SVM models. The
 601 top five rank features were β_0 , Parity, MAD_{dtrd} , Gestation,
 602 and Maternal Age based on their maximum relevance and min-
 603 imum redundancy. This is further confirmed by the minimum
 604 correlation shown among these features in the correlation plot
 605 shown in Fig. 4b. These features were next combined with the
 606 FHR times series using a deep learning model. This Fusion
 607 ResNet model trained on a large dataset of 9,887 FHR records,
 608 showed a superior AUC performance of 0.84 compared to the
 609 SVM models and the current state-of-the-art MCNN model
 610 performance in the benchmark CTU-UHB dataset.

611 The availability of a large training dataset ($n=9,887$) enabled
 612 us to train the proposed model and evaluate its performance
 613 on the external CTU-UHB dataset ($n = 552$), allowing for
 614 a fair comparison with previous studies that used the same
 615 benchmark. This approach reduces potential bias associated
 616 with training and reporting results on small or locally sourced
 617 datasets, while also demonstrating the model's robustness
 618 across diverse populations. For example, Spilka *et al.* [33] em-
 619 ployed a Sparse-SVM trained on three features (β_0 , MAD_{dtrd} ,
 620 and H) derived from the Lyon database consisting of 1,288
 621 recordings, achieving an AUC of 0.79 on a CTU-UHB subset
 622 with less than 50 percent signal loss. Ogasawara *et al.* [19]
 623 trained a CNN using FHR and UC time series data from
 624 a private dataset of 2,116 recordings from Keio University
 625 Hospital and reported a mean AUC of 0.68 on a CTU-UHB
 626 subset with signal loss below 16 percent. McCoy *et al.* [34]
 627 conducted a comparative study of six deep-learning models
 628 trained on a private dataset of 10,182 FHR recordings with
 629 less than 30 percent signal loss. Their best-performing model,
 630 InceptionTime, achieved AUCs of 0.76 and 0.72 on CTU-UHB
 631 with and without transfer learning, respectively. Another recent
 632 study evaluated a CNN model using a multicenter retrospective
 633 database comprising cases from three teaching hospitals of
 634 Assistance Publique des Hôpitaux de Paris (APHP), SpAM
 635 (Workshop on Signal Processing and Monitoring in Labor),
 636 and CTU-UHB, and found that it outperformed transformer-
 637 based models. The CNN achieved an AUC of 0.74 (90% CI:
 638 0.67–0.81) on the CTU-UHB dataset when trained on the other

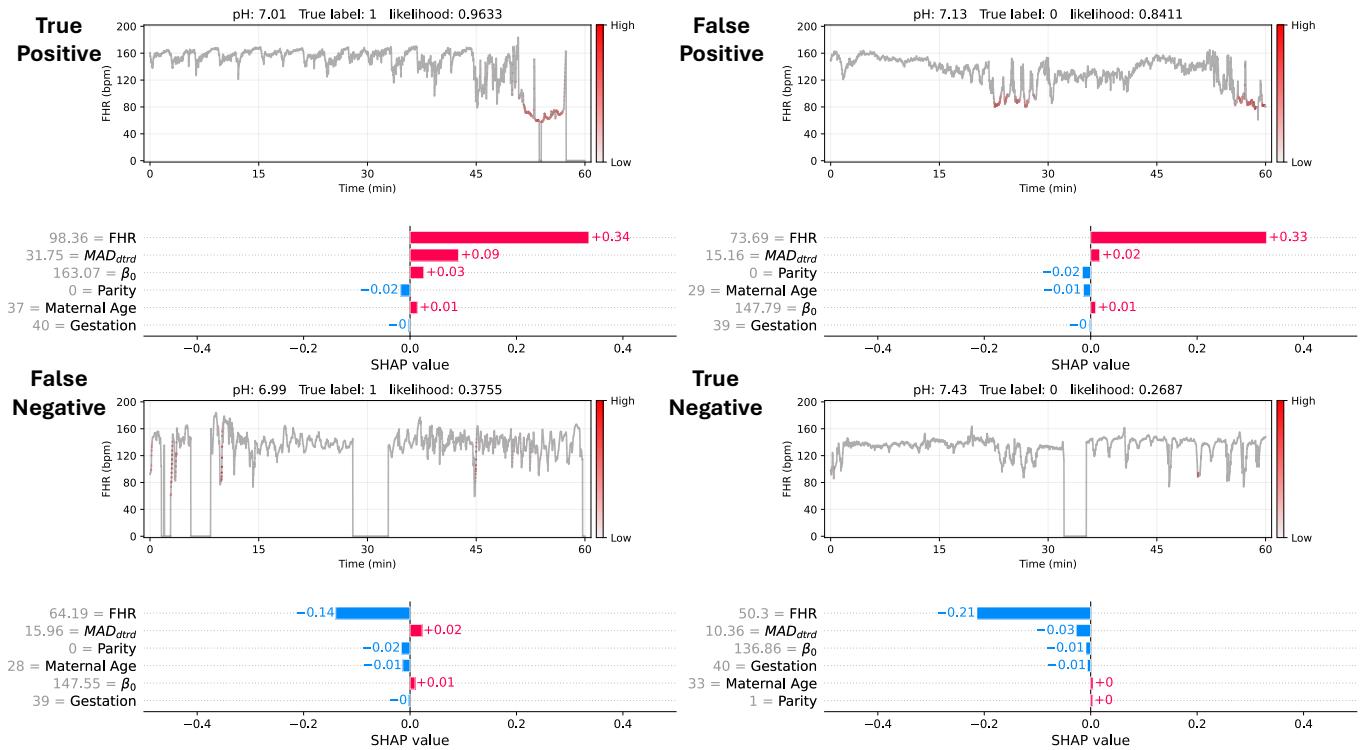


Fig. 8. The Grad-CAM and SHAP bar plots for true positive, false positive, false negative, and true negative cases. The Grad-CAM highlights FHR regions that strongly impact the model output. The SHAP bar plots show the tabular feature contributions to the model output.

639 four cohorts. Petrozziello et al. [7] proposed two deep learning
640 architectures, the MCNN and a stacked MCNN, which achieved
641 state-of-the-art AUCs of 0.81 and 0.82 respectively on the CTU-
642 UHB. However, the authors noted that MCNN performed better
643 than the stacked MCNN in their internal testing. These models
644 were trained on a dataset of over 35,000 CTG recordings using
645 FHR, UC, and a quality feature vector based on signal loss
646 percentage.

647 The main limitation of these existing studies is that they do
648 not integrate clinical parameters that are known to adversely af-
649 fect fetal outcomes as fetal compromise is rare, heterogeneous,
650 and challenging to detect with each fetal injury resulting from
651 a complex, multifactorial interaction [7], [35]. For instance, a
652 study analyzing 2,241 term singleton pregnancies observed
653 that nulliparity was significantly frequent in fetal acidosis
654 cases whereas no relationship was observed with gestational
655 diabetes and hypertension [36]. A prospective database of over
656 35,000 women from a multicenter investigation of singletons
657 showed a significant association with miscarriage, chromoso-
658 mal abnormalities, congenital anomalies, gestational diabetes,
659 placenta previa, and cesarean delivery with increasing maternal
660 age, and an increased risk of low birth weight and perinatal
661 mortality in women aged ≥ 40 years [37]. Similarly, other
662 retrospective studies have also shown that thick meconium,
663 gestational diabetes, and hypertensive disorders are associated
664 with adverse fetal outcomes [38], [39]. Petrozziello et al. [7]
665 in their study, suggested that combining deep learning with
666 domain-specific knowledge in future studies may improve the
667 detection of fetal compromise.

668 Only a few studies have explored the integration of clin-

ical features into prediction models for fetal compromise.
669 O'Sullivan et al. [13] incorporated parity, gestation, and hy-
670 pertension into a logistic regression model alongside CTG
671 features, which improved AUC performance from 0.79 to 0.82
672 in a 5-fold cross-validation on a subset of CTU-UHB data
673 ($n = 333$), where at-risk cases were defined by $pH \leq 7.0$
674 and Apgar score at 5 minutes ≤ 6 . Including the durations
675 of Stage 1 and Stage 2 labor further increased the AUC to
676 0.83 and 0.86, respectively. However, these durations are only
677 available during labor or retrospectively in the case of Stage
678 2 duration and thus are not suitable for real-time prediction.
679 Similarly, Houze de l'Aulnoit et al. [36] used a logistic
680 regression model combining FHR and clinical features (parity,
681 gestational age, fetal sex, and time from recording to delivery)
682 to predict acidosis ($pH \leq 7.15$), achieving an AUC of 0.79 in
683 a retrospective analysis of 2,241 singleton deliveries. A more
684 recent study introduced DeepCTG® 1.5 [14], which applied
685 logistic regression to integrate CTG features with clinical data
686 (maternal age, fetal growth restriction, diabetes, hypertension,
687 and meconium), showing an AUC of 0.71 compared to 0.70
688 when using CTG features alone. This model was trained on
689 a private dataset of 1,264 cases and evaluated on a subset of
690 CTU-UHB ($n = 550$) using $pH < 7.05$ as the outcome criterion.
691

692 In the present study, the Sparse SVM and Classical SVM
693 performance in multivariate feature analysis reached maximum
694 performance with only the top three features (β_0 , Parity, and
695 MAD_{dtrd}) in 5-fold CV on the MHW-pH dataset with both
696 models achieving a mean AUC of 0.69. When more features
697 were added, the Classical SVM performance degraded while the
698 Sparse SVM maintained a relatively similar performance. This

TABLE V
PERFORMANCE COMPARISON OF DEEP LEARNING MODELS IN PRIOR STUDIES EXTERNALLY TESTED ON THE CTU-UHB.

Study	DL Model	Input	Outcome	Training Dataset	Testing Dataset	AUC
Petrozziello et al., 2019 [7]	Stacked MCNN	FHR+UC+Quality	pH<7.05	Last 60 min of Stage 1 and the last 30 min of Stage 2 Oxford at 0.25 Hz	CTU-UHB	0.82
Petrozziello et al., 2019 [7]	MCNN	FHR+UC+Quality	pH<7.05	Last 60 min Oxford at 0.25 Hz	CTU-UHB	0.81
Ogasawara et al., 2021 [19]	CNN	FHR+UC	pH<7.05 or Apgar1<7	Last 30 min Keio data at 1 Hz	CTU-UHB (subset of 78 cases)	0.68 ± 0.03
McCoy et al., 2024 [34]	Inception Time	FHR	pH<7.05	Last 60 min Pennsylvania at 0.25 Hz	CTU-UHB	0.72
Ben M'Barek et al., 2025 [24]	CNN	FHR+UC	pH<7.05	Last 60 min Multicenter APHP + SPaM at 1 Hz	CTU-UHB	0.74 (90% CI: 0.67–0.81)
Mendis et al., 2025 [10]	ResNet	FHR	pH<7.05	Last 60 min MHW-pH at 1 Hz	CTU-UHB	0.81 ± 0.01
This Work	Fusion ResNet	FHR + Top 4 Tabular Features	pH<7.05	Last 60 min MHW-pH at 1 Hz	CTU-UHB	0.84 ± 0.02

699 can be attributed to the capability of sparse selection of weights
700 and features by the Sparse SVM model, effectively not selecting
701 underperforming features [9]. The trend of the first three
702 features achieving the optimum performance was consistent
703 with the external CTU-UHB evaluation in both models where
704 Sparse SVM achieved an AUC of 0.75 while Classical SVM
705 achieved an AUC of 0.74. Similar findings were reported by
706 Spilka et al. [9], where they found β_0 , MAD_{dtrd} , and H as
707 the top three features among 20 features for fetal compromise
708 detection using Sparse-SVM, achieving an AUC of 0.79. The
709 performance differences compared to our SVM models may be
710 attributed to the use of $pH \leq 7.05$ as the outcome criterion, the
711 focus on the last 20 minutes of the first stage of labor, and the
712 selection of a CTU-UHB subset that excluded recordings with
713 more than 50% signal loss. Additionally, the H feature may not
714 have ranked among the top features in the MHW-pH dataset
715 due to its positive correlation with MAD_{dtrd} and DC_{PRSA} ,
716 as all three features capture aspects of FHR variability.

717 In the deep learning approach of the present study, the top
718 five tabular features were combined with the FHR time series
719 using a Fusion ResNet model for improving fetal compromise
720 detection. The internal evaluation using a 5-fold CV of the
721 proposed Fusion ResNet model on MHW-pH showed the
722 highest mean AUC of 0.77 with only the top four tabular
723 features (β_0 , Parity, MAD_{dtrd} , and Gestation) fused with
724 the time series FHR. This highest-performing model, when
725 externally tested with CTU-UHB, achieved a state-of-the-art
726 AUC of 0.84 (74% TPR at 20% FPR, 67% TPR at 15% FPR),
727 outperforming existing prediction models including the MCNN
728 (AUC=0.81) and stacked MCNN (AUC=0.82). Its performance
729 was also superior to typical clinical practice which generally
730 lies between TPR of 31% to 48% at 16% and 21% FPR [7],
731 [8]. A comparison of the performance of existing deep learning
732 approaches and current work is given in Table V. The mean
733 area under the precision-recall curve (AUPRC), mean F1 scores
734 at 5, 10, 15, and 20% FPR of our selected model on CTU-UHB
735 were 0.39, 0.43, 0.40, 0.37, and 0.33, respectively. We refer

736 the reader to the supplementary materials for additional results
737 of AUPRC and F1 scores.

738 The superior performance of our Fusion ResNet model can
739 be attributed to its ability to integrate domain and clinical
740 knowledge captured in tabular features with complex, non-
741 linear patterns learned from the FHR time series. In clinical
742 practice, these tabular features including EHR features such as
743 Parity and Gestation are readily accessible to support informed
744 decision-making, while FHR features such as β_0 and MAD_{dtrd}
745 representing baseline and variability metrics are consistent
746 with FIGO guidelines for fetal monitoring and clinical as-
747 sessment. Furthermore, the Fusion ResNet model performance
748 was superior to both SVM models, demonstrating that deep
749 learning outperforms classical machine learning methods for
750 fetal compromise detection as identified by existing works
751 [17], [19]. Another advantage of the Fusion ResNet model is
752 the ability of its FHR time-series branch to process variable
753 input lengths, which enhances its suitability for real-world
754 deployment. This flexibility is achieved through the use of
755 a ResNet architecture followed by a global average pooling
756 layer in the FHR branch [10]. This design also contributes to
757 the model's low computational overhead, primarily achieved
758 through the use of 1D convolutions, a global average pooling
759 layer that eliminates the need for large dense layers, and a
760 lightweight tabular branch consisting of two fully connected
761 layers. The selected model contained 505,587 trainable param-
762 eters and required 3.6 GFLOPs per 60-minute FHR segment.
763 The mean inference time per 60-minute segment was 15.33 ms
764 on an NVIDIA A100 GPU and 76.44 ms on a standard
765 Intel Core i7-1185G7 CPU. These architectural choices ensure
766 that the proposed model remains computationally efficient
767 and suitable for real-time deployment in intrapartum fetal
768 monitoring systems.

769 A further limitation of previous ML and DL studies for
770 FHR evaluation was the limited explainability of the model
771 predictions. Clinicians often express reluctance to adopt
772 predictive ML and DL models due to limited transparency

773 regarding how input features contribute to the model's decision-
774 making process [40], [41]. This lack of interpretability hinders
775 clinical trust and restricts integration into routine practice,
776 particularly in high-stakes settings such as intrapartum care.
777 The present study addressed this limitation by investigating
778 the interpretability of the deep learning model fused with
779 the top five tabular features using two explainable artificial
780 intelligence techniques: Grad-CAM and SHAP. A previous
781 study by our research group [10] used CAM to explain the
782 model predictions, but to the best of our knowledge, this is the
783 first study to use both methods to explain a model used for
784 fetal compromise detection. The global SHAP values shown
785 by the beeswarm plot in Fig. 7 demonstrate that higher feature
786 values of all features except for Gestation contribute highly
787 to the likelihood of fetal compromise. Particularly, this aligns
788 with domain knowledge where high maternal age, high FHR
789 baseline (β_0), and longer depth of decelerations (MAD_{dtrd}) are
790 associated with fetal compromise [4], [33], [37]. Furthermore,
791 the ability of Grad-CAM to identify regions of high importance
792 and SHAP values to show feature importance in explaining
793 individual case predictions of true positive, false positive, true
794 negative, and false negative were illustrated. These visual
795 representations, if made available during the clinical decision-
796 making process, could offer valuable insights that support more
797 informed, reliable, and accurate assessment by clinicians.

798 Interestingly, both the SVM and deep learning models
799 showed reduced performance when Parity was added to the β_0
800 feature when tested on the CTU-UHB dataset. This pattern was
801 not observed during the 5-fold cross-validation on the MHW-
802 pH dataset. A possible explanation is the higher proportion
803 of nulliparous compromised cases in the CTU-UHB dataset
804 compared to the training distribution in the MHW-pH dataset,
805 as shown in Fig. 4a. Previous studies have reported a consistent
806 association between nulliparity and fetal compromise [36].
807 Similarly, significant differences between Normal and Compro-
808 mised cases were also observed in both MHW-pH and CTU-
809 UHB datasets. However, the low prevalence of compromised
810 cases (1.1%) and the small number of nulliparous cases within
811 the compromised group in the MHW-pH dataset may have
812 limited the model's ability to learn from this feature during
813 training. This is also reflected in the low SHAP values observed
814 for low Parity cases. The negative impact was offset when
815 MAD_{dtrd} was included, demonstrating its strong contribution
816 to model predictions. This is further supported by the higher
817 SHAP values of MAD_{dtrd} compared to other tabular features,
818 as shown in Fig. 7.

819 Another important observation was that both the SVM
820 models and the Fusion ResNet models performed better on the
821 external testing set CTU-UHB than on the internal validation
822 set MHW-pH. Similar trends have been reported in previous
823 studies that externally evaluated model performance on CTU-
824 UHB [7], [10], [33]. One possible explanation is that the
825 CTU-UHB dataset is smaller and less heterogeneous, with
826 data collected over a period of less than three years and a
827 high prevalence of fetal compromise (7.2%). In contrast, the
828 MHW-pH dataset is approximately 18 times larger, spanning
829 12 years of clinical practice, and reflects a low prevalence rate
830 of 1.1%. These differences highlight the importance of vali-

831 dating predictive models on large, diverse, and representative
832 datasets. Overreliance on smaller, less heterogeneous cohorts
833 may lead to an overestimation of model performance and limit
834 generalizability in real-world clinical settings.

V. LIMITATIONS AND FUTURE WORK

835 This study has several limitations. First, the tabular feature
836 set was limited to twelve tabular features, including six EHR
837 features selected based on their availability in both datasets
838 and four human-crafted FHR features identified from previous
839 studies. Because the recordings were not pre-filtered for signal
840 loss, the handcrafted FHR features extracted using classical
841 methods may have been affected. Second, feature selection was
842 limited to the mRMR method, and future work could extend
843 this to compare other feature selection methods, including
844 strategies embedded within neural networks. Third, several of
845 the features used in this study have previously been identified
846 as predictive within the CTU-UHB dataset, as demonstrated
847 in the work by Spilka et al. [33]. Since the proposed model
848 was developed and validated using only the MHW-pH and
849 CTU-UHB datasets, representing cohorts from Australia and
850 the Czech Republic, its generalizability to broader populations
851 needs to be confirmed. Fourth, although the model achieved a
852 TPR of 67–72% at a 15–20% FPR on the external CTU-UHB
853 dataset, surpassing typical clinician performance of 31–48%
854 TPR at 16–21% FPR [7], [8], this trade-off between sensitivity
855 and specificity must be carefully considered for real-world
856 deployment. While higher sensitivity is desirable for timely
857 intervention, further improvement in specificity will reduce
858 unnecessary cesarean sections and alarm fatigue in practice.
859 Fifth, while the SHAP and Grad-CAM explanations demon-
860 strate strong alignment with known physiological patterns,
861 their clinical plausibility warrants validation through expert
862 consultation. Future work will involve collaboration with
863 obstetricians to review interpretability maps and conduct case-
864 based clinical evaluations. Therefore, further validation in more
865 diverse retrospective datasets and prospective clinical trials is
866 needed to assess the generalizability of the proposed model
867 and to determine whether its integration into clinical practice
868 can lead to improved fetal outcomes.

VI. CONCLUSION

870 In conclusion, this cross-center study involving over 10,000
871 FHR recordings demonstrates that integrating domain-specific
872 and clinical features with FHR time series data using deep
873 learning significantly enhances the detection of fetal com-
874 promise. The proposed Fusion ResNet model achieved state-
875 of-the-art performance, with an AUC of 0.84 on the open-
876 access CTU-UHB dataset. For the first time, model predictions
877 were interpreted using two explainable artificial intelligence
878 techniques, providing visual insights into the contribution of
879 both tabular features and FHR signal regions to the model's
880 output. These approaches enhance clinical interpretability
881 and may help address concerns among clinicians regarding
882 the perceived lack of transparency in deep learning models,
883 thereby improving their clinical acceptability. The improved
884 predictive performance and interpretability of the proposed

886 method represent a step toward the development of a robust
887 computerized CTG analysis system with the potential to reduce
888 adverse perinatal outcomes.

889 ACKNOWLEDGMENT

890 L. Mendis is supported by the Melbourne Research Scholarship
891 and a Top-Up Scholarship from the Graeme Clark Institute
892 for Biomedical Engineering at the University of Melbourne. E.
893 Keenan is supported by an Early Career Research Fellowship
894 from the Department of Obstetrics and Gynaecology at the
895 University of Melbourne. F. Brownfoot is supported by an
896 NHMRC Early Career Fellowship (NHMRC #1142636) and a
897 Norman Beischer Clinical Research Fellowship. D. Karmakar
898 is supported by an NHMRC postgraduate scholarship. This
899 research was supported by The University of Melbourne's
900 Research Computing Services and the Petascale Campus Initiative.

902 CONFLICT OF INTEREST

903 E. Keenan, M. Palaniswami, and F. Brownfoot are co-
904 founders and shareholders of Kali Healthcare Pty Ltd. L.
905 Mendis and D. Karmakar have no competing interests to
906 declare.

907 REFERENCES

- [1] United Nations Inter-agency Group for Child Mortality Estimation (UN IGME), "Never Forgotten: The situation of stillbirth around the globe," United Nations Children's Fund, New York, Report, 2023.
- [2] R. L. Goldenberg, M. S. Harrison, and E. M. McClure, "Stillbirths: The Hidden Birth Asphyxia - US and Global Perspectives," *Clinics in Perinatology*, vol. 43, no. 3, pp. 439–453, Sep. 2016.
- [3] A. Pinas and E. Chandraharan, "Continuous cardiotocography during labour: Analysis, classification and management," *Best Practice & Research Clinical Obstetrics & Gynaecology*, vol. 30, pp. 33–47, Jan. 2016.
- [4] D. Ayres-de Campos *et al.*, "FIGO consensus guidelines on intrapartum fetal monitoring: Cardiotocography," *International Journal of Gynecology & Obstetrics*, vol. 131, no. 1, pp. 13–24, 2015.
- [5] L. Hrulan *et al.*, "Agreement on intrapartum cardiotocogram recordings between expert obstetricians," *Journal of Evaluation in Clinical Practice*, vol. 21, no. 4, pp. 694–702, Aug. 2015.
- [6] Z. Alfirevic *et al.*, "Continuous cardiotocography (CTG) as a form of electronic fetal monitoring (EFM) for fetal assessment during labour," *Cochrane Database of Systematic Reviews*, no. 2, 2017.
- [7] A. Petrozziello *et al.*, "Multimodal Convolutional Neural Networks to Detect Fetal Compromise During Labor and Delivery," *IEEE Access*, vol. 7, pp. 112026–112036, 2019.
- [8] P. Abry *et al.*, "Sparse learning for Intrapartum fetal heart rate analysis," *Biomedical Physics & Engineering Express*, vol. 4, no. 3, p. 034002, Apr. 2018.
- [9] J. Spilka *et al.*, "Sparse Support Vector Machine for Intrapartum Fetal Heart Rate Classification," *IEEE Journal of Biomedical and Health Informatics*, vol. 21, no. 3, pp. 664–671, May 2017.
- [10] L. Mendis *et al.*, "Cross-Database Evaluation of Deep Learning Methods for Intrapartum Cardiotocography Classification," *IEEE Journal of Translational Engineering in Health and Medicine*, pp. 1–1, 2025.
- [11] A. Georgieva, C. W. G. Redman, and A. T. Papageorgiou, "Computerized data-driven interpretation of the intrapartum cardiotocogram: a cohort study," *Acta Obstetricia Et Gynecologica Scandinavica*, vol. 96, no. 7, pp. 883–891, Jul. 2017.
- [12] L. Mendis *et al.*, "Computerised Cardiotocography Analysis for the Automated Detection of Fetal Compromise during Labour: A Review," *Bioengineering*, vol. 10, no. 9, p. 1007, Sep. 2023.
- [13] M. O'Sullivan *et al.*, "Classification of fetal compromise during labour: signal processing and feature engineering of the cardiotocograph," in *2021 29th European Signal Processing Conference (EUSIPCO)*, Dublin, Ireland, Aug. 2021, pp. 1331–1335.
- [14] E. Menzhulina *et al.*, "Integration of clinical features in a computerized cardiotocography system to predict severe newborn acidemia," *European Journal of Obstetrics & Gynecology and Reproductive Biology*, vol. 307, pp. 78–83, Apr. 2025.
- [15] A. Georgieva *et al.*, "Phase-rectified signal averaging for intrapartum electronic fetal heart rate monitoring is related to acidemia at birth," *BJOG: An International Journal of Obstetrics & Gynaecology*, vol. 121, no. 7, pp. 889–894, 2014.
- [16] A. Lovers *et al.*, "Advancements in Fetal Heart Rate Monitoring: A Report on Opportunities and Strategic Initiatives for Better Intrapartum Care," *BJOG: An International Journal of Obstetrics & Gynaecology*, vol. n/a, no. n/a, 2025.
- [17] L. Mendis *et al.*, "Rapid detection of fetal compromise using input length invariant deep learning on fetal heart rate signals," *Scientific Reports*, vol. 14, no. 1, p. 12615, Jun. 2024.
- [18] A. Petrozziello *et al.*, "Deep Learning for Continuous Electronic Fetal Monitoring in Labor," in *2018 40th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC)*, Honolulu, HI, USA, Jul. 2018, pp. 5866–5869.
- [19] J. Ogasawara *et al.*, "Deep neural network-based classification of cardiotograms outperformed conventional algorithms," *Scientific Reports*, vol. 11, no. 1, p. 13367, Jun. 2021.
- [20] D. Karmakar *et al.*, "Impact of missing electronic fetal monitoring signals on perinatal asphyxia: a multicohort analysis," *npj Digital Medicine*, vol. 8, no. 1, pp. 1–9, May 2025.
- [21] R. Pardasani *et al.*, "Development of a novel artificial intelligence algorithm for interpreting fetal heart rate and uterine activity data in cardiotocography," *Frontiers in Digital Health*, vol. 7, Sep. 2025.
- [22] M. J. Khan, M. Vatish, and G. Davis Jones, "PatchCTG: A Patch Cardiotocography Transformer for Antepartum Fetal Health Monitoring," *Sensors*, vol. 25, no. 9, p. 2650, Jan. 2025.
- [23] K. E. Gumilar *et al.*, "Artificial intelligence-large language models (AI-LLMs) for reliable and accurate cardiotocography (CTG) interpretation in obstetric practice," *Computational and Structural Biotechnology Journal*, vol. 27, pp. 1140–1147, Mar. 2025.
- [24] I. Ben M'Barek *et al.*, "DeepCTG® 2.0: Development and validation of a deep learning model to detect neonatal acidemia from cardiotocography during labor," *Computers in Biology and Medicine*, vol. 184, p. 109448, 2025.
- [25] V. Chudáček *et al.*, "Open access intrapartum CTG database," *BMC Pregnancy and Childbirth*, vol. 14, no. 1, p. 16, Jan. 2014.
- [26] J. Spilka *et al.*, "Automatic Evaluation of FHR Recordings from CTU-UHB CTG Database," in *Proceedings of the 4th International Conference, ITBAM 2013*, M. Bursa, S. Khuri, and M. E. Renda, Eds. Prague, Czech Republic: Springer, Berlin, Heidelberg, 2013, pp. 47–61.
- [27] J. Spilka, "Complex approach to fetal heart rate analysis: A hierarchical classification model," Ph.D dissertation, Czech Technical University in Prague, Faculty of Electrical Engineering, Department of Cybernetics, 2013.
- [28] Z. Zhao *et al.*, "DeepFHR: intelligent prediction of fetal Acidemia using fetal heart rate signals based on convolutional neural network," *BMC Medical Informatics and Decision Making*, vol. 19, no. 1, p. 286, Dec. 2019.
- [29] C. Ding and H. Peng, "Minimum redundancy feature selection from microarray gene expression data," in *Computational Systems Bioinformatics. CSB2003. Proceedings of the 2003 IEEE Bioinformatics Conference. CSB2003*, Aug. 2003, pp. 523–528.
- [30] P. A. Warrick *et al.*, "Classification of Normal and Hypoxic Fetuses From Systems Modeling of Intrapartum Cardiotocography," *IEEE Transactions on Biomedical Engineering*, vol. 57, no. 4, pp. 771–779, Apr. 2010.
- [31] R. R. Selvaraju *et al.*, "Grad-CAM: Visual Explanations from Deep Networks via Gradient-Based Localization," *International Journal of Computer Vision*, vol. 128, no. 2, pp. 336–359, Feb. 2020.
- [32] S. M. Lundberg and S.-I. Lee, "A unified approach to interpreting model predictions," in *Proceedings of the 31st International Conference on Neural Information Processing Systems*, ser. NIPS'17. Red Hook, NY, USA: Curran Associates Inc., Dec. 2017, pp. 4768–4777.
- [33] J. Spilka *et al.*, "Intrapartum Fetal Heart Rate Classification: Cross-Database Evaluation," in *Proceedings of the XIV Mediterranean Conference on Medical and Biological Engineering and Computing 2016*, ser. IFMBE Proceedings, E. Kyriacou, S. Christofides, and C. S. Pattichis, Eds. Paphos, Cyprus: Springer, Cham, 2016, pp. 1199–1204.
- [34] J. A. Mccoy *et al.*, "Intrapartum electronic fetal heart rate monitoring to predict acidemia at birth with the use of deep learning," *American Journal of Obstetrics & Gynecology*, vol. 0, no. 0, Apr. 2024.

- 1025 [35] J. M. Turner, M. D. Mitchell, and S. S. Kumar, "The physiology of
1026 intrapartum fetal compromise at term," *American Journal of Obstetrics & Gynecology*, vol. 222, no. 1, pp. 17–26, Jan. 2020.
1027
1028 [36] A. Houzé de l'Aulnoit *et al.*, "Use of automated fetal heart rate analysis
1029 to identify risk factors for umbilical cord acidosis at birth," *Computers in Biology and Medicine*, vol. 115, p. 103525, Dec. 2019.
1030
1031 [37] J. Cleary-Goldman *et al.*, "Impact of Maternal Age on Obstetric Outcome,"
1032 *Obstetrics & Gynecology*, vol. 105, no. 5 Part 1, p. 983, May 2005.
1033
1034 [38] O. Gluck *et al.*, "The effect of meconium thickness level on neonatal
1035 outcome," *Early Human Development*, vol. 142, p. 104953, Mar. 2020.
1036
1037 [39] Y.-W. Lin *et al.*, "Population-based study on birth outcomes among
1038 women with hypertensive disorders of pregnancy and gestational diabetes
1039 mellitus," *Scientific Reports*, vol. 11, no. 1, p. 17391, Aug. 2021.
1040
1041 [40] R. Dlugatch, A. Georgieva, and A. Kerasidou, "AI-driven decision support
1042 systems and epistemic reliance: a qualitative study on obstetricians'
1043 and midwives' perspectives on integrating AI-driven CTG into clinical
1044 decision making," *BMC Medical Ethics*, vol. 25, no. 1, p. 6, Jan. 2024.
1045
1046 [41] A. Vellido, "The importance of interpretability and visualization in
1047 machine learning for applications in medicine and health care," *Neural Computing and Applications*, vol. 32, no. 24, pp. 18 069–18 083, Dec.
1048 2020.
1049