



The effects of anastomosis angle on blood flow in bypassed blood vessel

이건우¹, #이경은¹

¹ 인하대학교 기계공학과

Kunwoo Lee¹, #Kyung Eun Lee¹(bfmec@inha.ac.kr)

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¹ Department of Mechanical Engineering, Inha University, Republic of Korea

Introduction

- ❖ Severe atherosclerosis have been treated with vascular bypass surgery.
- ❖ It is known that wall shear stress effects on the patency of surgery.
- ❖ Aim of this study: to understand the correlation between anastomosis angle and wall shear stress distributions in a totally occluded vessel.

Figure 1. Development of Atherosclerosis
Image source : UR Medicine

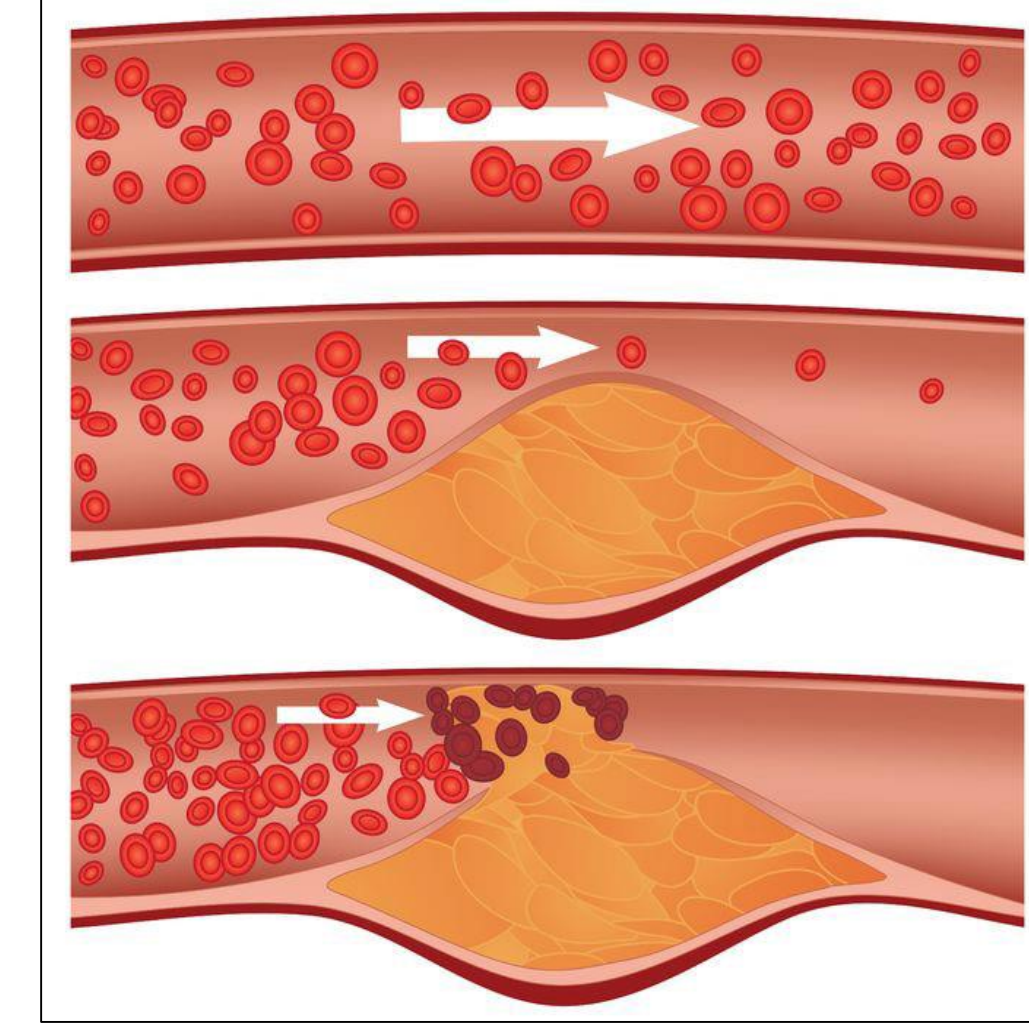
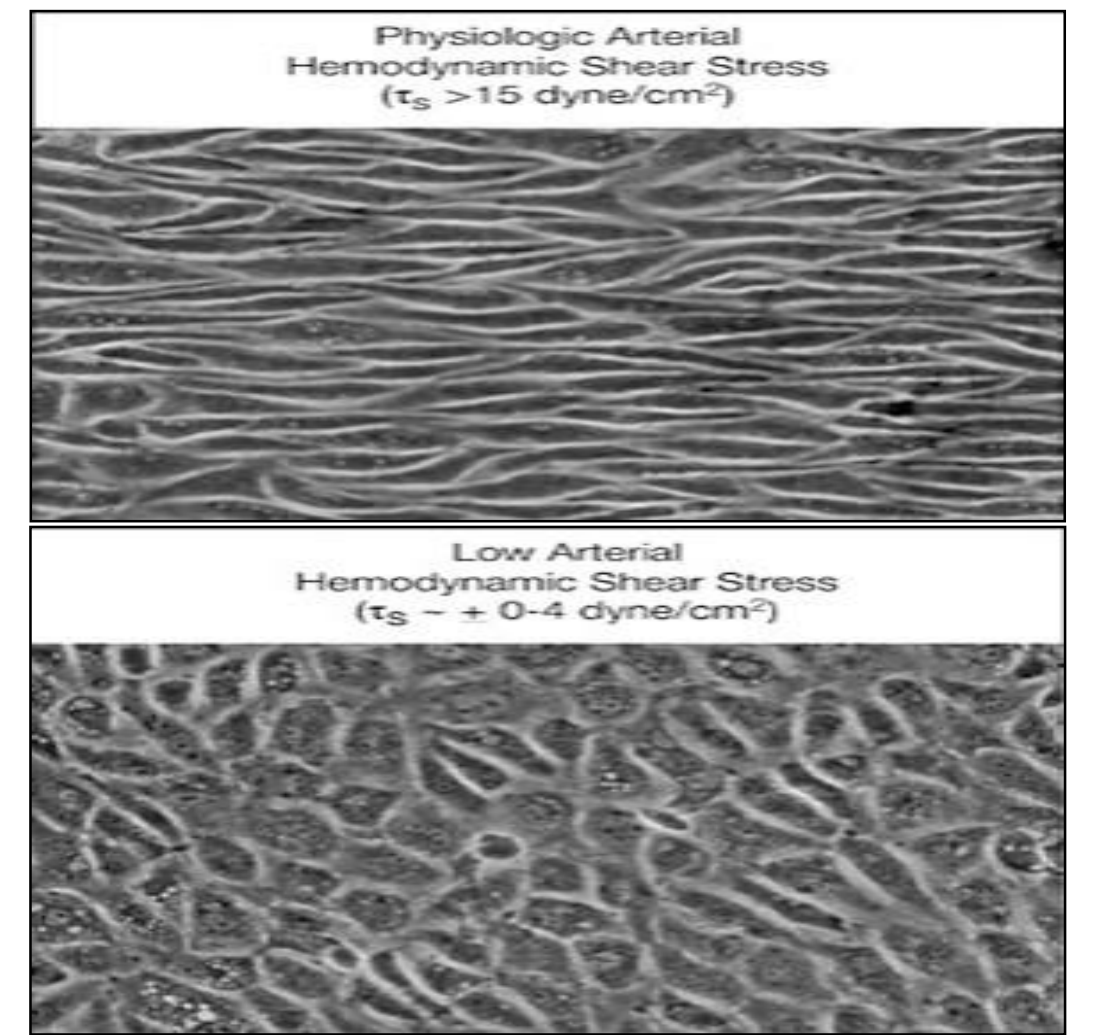
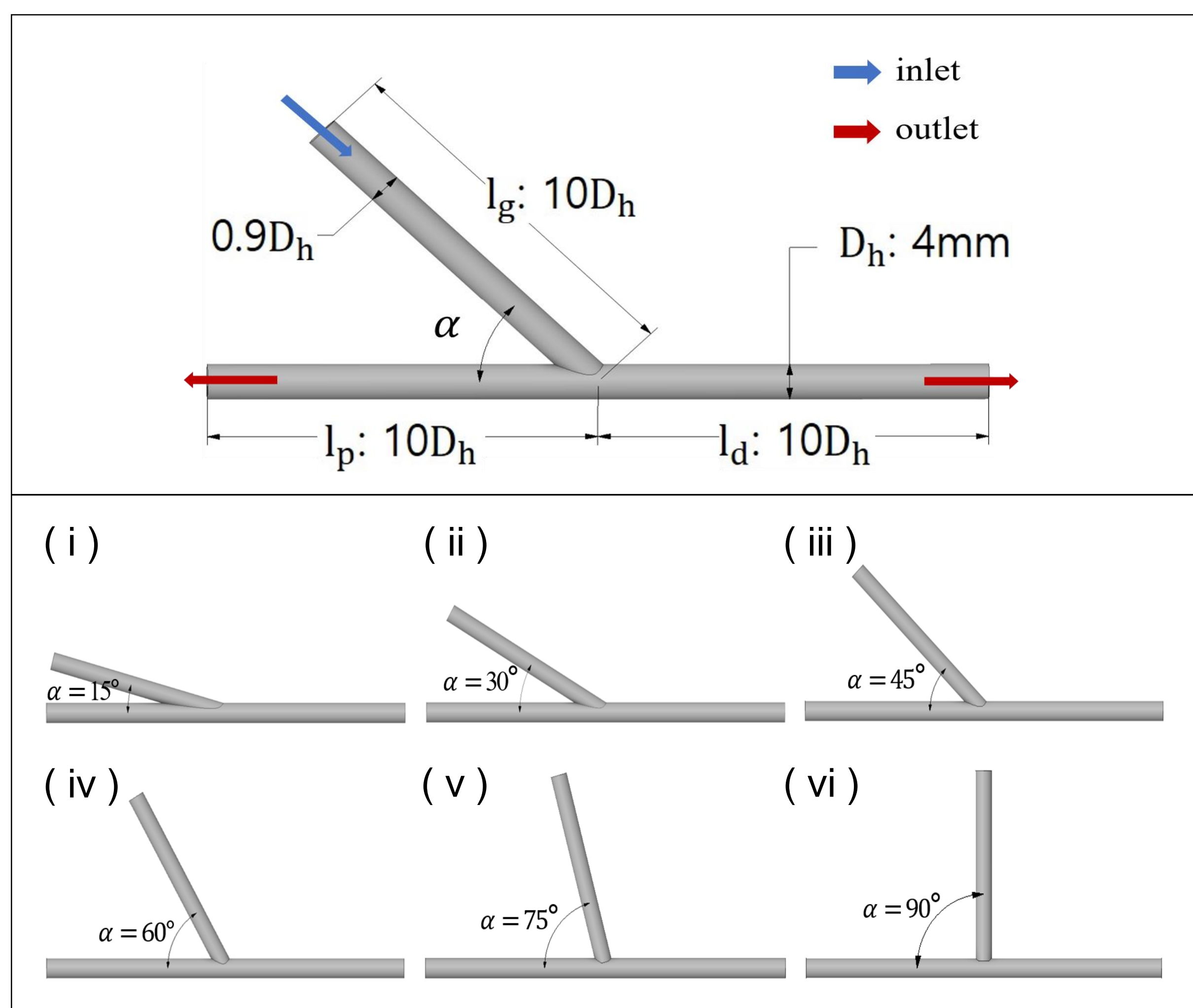


Figure 2. Endothelial Cell Morphology according to Shear Stress level
Image source : Malek et al. "Hemodynamic Shear Stress and its Role in Atherosclerosis"



Modeling

Figure 3. Dimensions of model i ~ vi : anastomosis angle (α) 15° ~ 90° with 15° interval



Governing Equations

• Continuity Equation $\frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} + \frac{\partial w}{\partial z} = 0$

• Navier-Stokes Equation of Incompressible Newtonian Fluid

$$\begin{aligned} \rho g_x - \frac{\partial p}{\partial x} + \mu \left(\frac{\partial^2 u}{\partial x^2} + \frac{\partial^2 u}{\partial y^2} + \frac{\partial^2 u}{\partial z^2} \right) &= \rho \left(\frac{\partial u}{\partial t} + u \frac{\partial u}{\partial x} + v \frac{\partial u}{\partial y} + w \frac{\partial u}{\partial z} \right) \\ \rho g_y - \frac{\partial p}{\partial y} + \mu \left(\frac{\partial^2 v}{\partial x^2} + \frac{\partial^2 v}{\partial y^2} + \frac{\partial^2 v}{\partial z^2} \right) &= \rho \left(\frac{\partial v}{\partial t} + u \frac{\partial v}{\partial x} + v \frac{\partial v}{\partial y} + w \frac{\partial v}{\partial z} \right) \\ \rho g_z - \frac{\partial p}{\partial z} + \mu \left(\frac{\partial^2 w}{\partial x^2} + \frac{\partial^2 w}{\partial y^2} + \frac{\partial^2 w}{\partial z^2} \right) &= \rho \left(\frac{\partial w}{\partial t} + u \frac{\partial w}{\partial x} + v \frac{\partial w}{\partial y} + w \frac{\partial w}{\partial z} \right) \end{aligned}$$

Numerical Analysis Method

- Finite Volume Method (Ansys Fluent 2021 R1)

Mesh

- Tetrahedral Mesh

| Number of Mesh | |
|--------------------------------------------------------------|--|
| Model i : 558,678 , Model ii : 326,014 , Model iii : 331,453 | |
| Model iv : 581,301 , Model v : 649,433 , Model vi : 662,149 | |

Assumptions

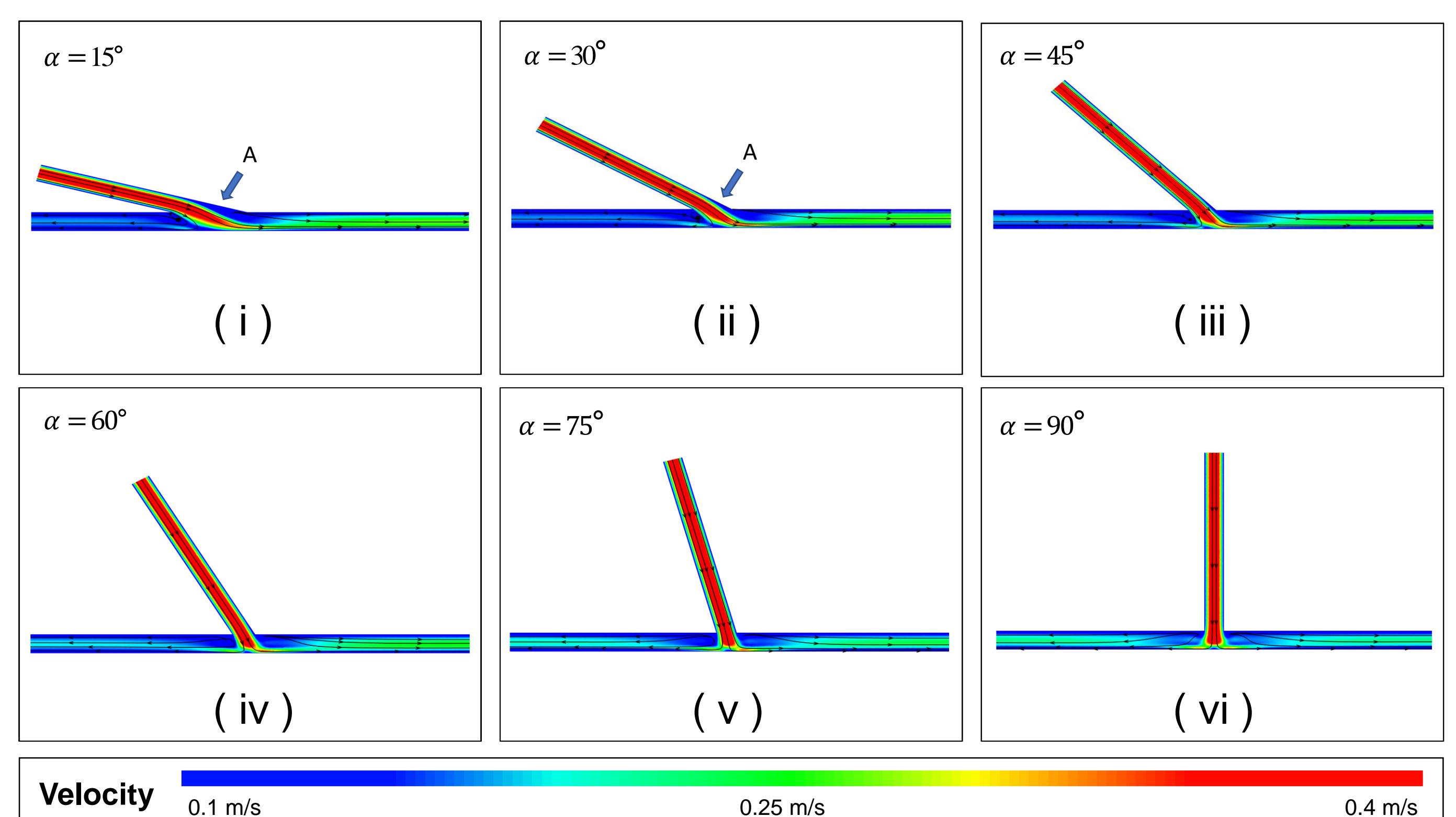
- Steady Flow, Incompressible Newtonian Fluid, Rigid Wall, No Gravitational Effect

Boundary Condition

- Inlet : $Re = 250$, $V_{avg} = 0.26984$ m/s , Fully Developed Laminar Flow
- Outlet : Neumann Boundary, Zero Traction

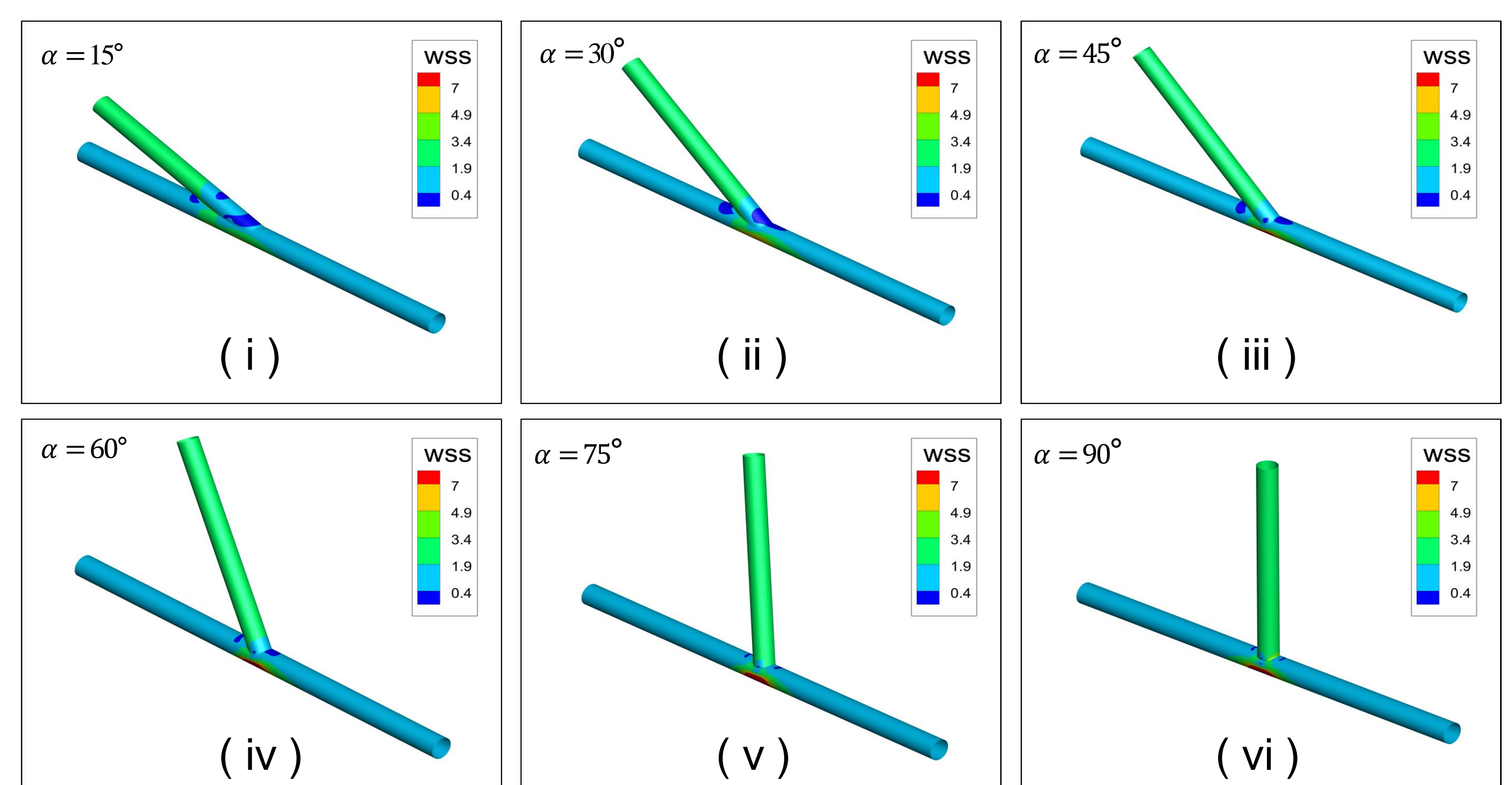
Result

Figure 4. Velocity Contour in Axial Section



- Flows with high velocity(above 0.3m/s) were not affected by anastomosis angle.
- Slow moving flows were observed in graft anastomosis(area A) in model i and ii (15° and 30°)
- Velocity in proximal area was faster in models with anastomosis angle above 45°, compared to models below 45°.
- Recirculating flow was formed in proximal anastomosis area in models with anastomosis angle below 45°.

Figure 5. Wall Shear Stress Distributions



- Low wall shear stress regions were observed near anastomosis in all models.
- The increase of anastomosis angle decreased the size of low wall shear stress region.

Conclusion

- ❖ As the size of low wall shear stress region decreases near anastomosis, increasing anastomosis angle may reduce the risk of restenosis near anastomosis.

Acknowledgments

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바이오 유체공학 연구실
Bio Fluid Engineering Laboratory (<http://bioflow.inha.ac.kr>)