

# ZebraSound : architecture and notes

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## 1 Introduction : notation and base principle

The sonification is based on the mean fluorescence signals computed over a set or ROI. An ROI (or neuron) is represented by an FM operator.

Mapping :

- Fluorescence : Amplitude
- Group parameter : Modulation index
- First derivative : harmonicity (not used, set to 1)

### 1.1 Notation

We note  $\mathbf{F}(n) = [f_0(n), \dots, f_i(n), \dots, f_{N_{ROI}-1}(n)]^T$  the vector containing the mean fluorescence in each ROI at the current frame  $n$ . The element  $f_i(n)$  designates the fluorescence associated with the  $i^{th}$  ROI.

We note  $\mathbf{G}(n) = [g_0(n), \dots, g_j(n), \dots, g_{N_G-1}(n)]^T$  the *group vector* which contains the parameters computed for each group  $j$ ,  $0 < j < N_G$ , with  $N_G$  the number of groups (nine in our case).

Therefore,  $\mathbf{G}(n)$  can be computed with a matrix operation :  $\mathbf{G}(n) = \mathbf{A} \cdot \mathbf{F}(n)$ , with  $\mathbf{A}$  a matrix of dimension  $N_G \times N_{ROI}$ . The coefficients of  $\mathbf{A}$  then determine which parameter is being computed. We note that  $\mathbf{G}(n)$  can be computed using the first time derivative or  $\mathbf{F}(n)$ .

Four parameter are currently implemented :

- Mean fluorescence in the group
- ratio of activated neurons
- first derivative of the above

These parameters can be computed either on the fluorescence or on its first derivative.

Due to the high dimensions of our data, we prefer direct computation of  $\mathbf{G}(n)$  over a costfull matrix operation.

The raw data goes through a preprocessing and a normalization. The resulting signal vectors are noted  $\mathbf{F}_p(n)$  and  $\mathbf{F}_n(n)$  respectively.

The scaled signals are notes with the subscript  $s$ , the driving signals are noted with the subscript  $d$ .

### 1.2 overall structure

The overall structure is represented figure 1.

**Amplitude driving<sup>1</sup>** The raw data go through the processing, which consists in a preprocessing and a normalization. Both are discussed in section 2. The normalized signal and its first derivative (backward finite differences,  $o(h^2)$ ). For each frame the current vector  $fn$  is obtained from the processed data to be used in the sonification.

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<sup>1</sup>synthesis

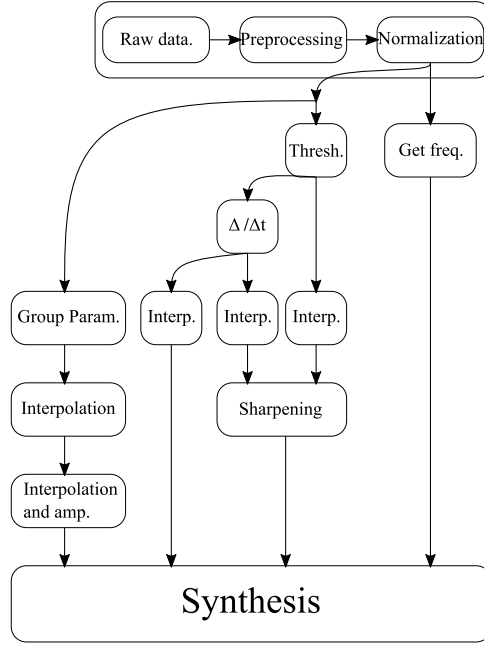


Figure 1: overview

The signal  $\mathbf{F}_{\mathbf{n}}(n)$  is threshed and scaled.  $\frac{d\mathbf{F}_{\mathbf{n}}(n)}{dt}$  is scaled and used to sharpen  $\mathbf{F}_{\mathbf{s}}(n)$  according to the expression

$$\mathbf{F}_{\mathbf{d}}(n) = (1 - a)\mathbf{F}_{\mathbf{s}}(n) + a \left[ \frac{d\mathbf{F}_{\mathbf{n}}(n)}{dt} \right]_s \quad (1)$$

Where  $a$  is an arbitrary coefficient, and  $[\cdot]_s$  designates the scaling operation.

As of march 29<sup>th</sup> the driving parameter is scaled according to the size of the ROI :

$$\mathbf{F}_{\mathbf{d}}(n) = \left[ (1 - a)\mathbf{F}_{\mathbf{s}}(n) + a \left[ \frac{d\mathbf{F}_{\mathbf{n}}(n)}{dt} \right]_s \right] \cdot \left[ \frac{\mathbf{size}}{size_{max}} \right]_s \quad (2)$$

Where  $size_{max}$  is the size (in pixel) of the largest ROI in the dataset.

**Modulation index driving** <sup>2</sup> The modulation is driven by the scaled group parameter multiplied by an arbitrary coefficient  $k$ , so that  $\mathbf{G}_{\mathbf{d}}(n) = k\mathbf{G}_{\mathbf{s}}(n)$ . The amplification by a factor  $k$  is used to set the range of variation of the modulation index. For each frame the values are routed and the parameter is computed. The computation is detailed in section 3.3.

**harmonicity driving** The harmonicity is driven by the scaled derivative of the signal, computed over three frames.

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<sup>2</sup>synthesis

**Frequency** The carrier frequency of each operator is obtained by referencing the cluster the neuron belongs to. The note associated with each group is set by the user.

As of march 29<sup>th</sup> the user can choose to double the frequency of the right hemisphere.

As of 04/23 an additionnal detune effect was added to explore differences of the group parameters computed in each hemisphere. The choice of the parameter is left to the user. The final frequency  $f$  is obtained with the relation [cite]

$$f = f_{note} \left( 1 \pm DF \left| \frac{Param_{left} - Param_{right}}{Param_{right}} \right|_s \right) \quad (3)$$

Where  $DF$  is set by the user.

## 2 Data processing<sup>3</sup>

In this section we detail the computation of the processed and the normalized signals.

### 2.1 Preprocessing

Two preprocessing methods are implemented, the *average* (eq. 4) and the *standard deviation* (eq. 5).

$$\mathbf{F}_p(n) = \frac{|\mathbf{F}(n) - f_{mean}|}{f_{mean}} \quad (4)$$

$$\mathbf{F}_p(n) = \frac{|\mathbf{F}(n) - \sigma^2|}{f_{mean}} \quad (5)$$

$f_{mean}$  designates the vector of size  $N_{ROI}$  which contains the mean fluorescence in each ROI, over the whole recording. Therefore it is expressed as

$$f_{mean} = [mean(f_0), ..., mean(f_i), ..., mean(f_{N_{ROI}-1})]^T \quad (6)$$

**output** The output of the synthesizer is equalized on a per group basis. Moreover, the user can choose to hear only tracked neurons (tracked neuron mode) or the tracked groups (tracked groups mode). This is done by setting to 0 the amplitude of the other neurons, prior to synthesis.

### 2.2 Normalization

In the case of the data obtained from FIJI, the fluorescence values are between 0 (black pixel) and 255 (white pixel). Therefore a straightforward normalization is obtained by dividing the whole data by 255. Two others normalization methods (computed over the data divided by 255) are implemented : the *maximum* (eq. 7) and *overall maximum* (eq. 8). Both of these can be bypassed.

$$\mathbf{F}_n(n) = \frac{\mathbf{F}_p(n)}{max(\mathbf{F}_p(n))} \quad (7)$$

$$\mathbf{F}_n(n) = \frac{\mathbf{F}_p(n)}{max_{whole}(\mathbf{F}_p(n))} \quad (8)$$

A vector containing the standard deviation of each signal is computed over the whole data  $fn$ . It is used in the threshold.

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<sup>3</sup>settings/data

### 3 Synthesis

In the section we detail the synthesis process, starting with the processing of the driving parameters. Then we detail the structure of a single operator and the computation of the group parameters.

#### 3.1 Parameter processing

Prior to entering the operator the frequency and  $\mathbf{F_d}(n)$  are processed. More specifically, the frequency is changed based on which hemisphere the neuron belongs to, and  $\mathbf{F_d}(n)$  goes through a karplus-strong digital waveguide.

In the first part we detail the processing outside of the poly object, and thus operating at control rate. In the second part we detail the signal rate processing.

##### 3.1.1 outside poly

The frequency and  $\mathbf{F_d}(n)$  are processed at control rate before entering the poly object.

**Frequency** Left and right hemisphere are discriminated using its  $x$  coordinate :

- $x < 0$  : left hemisphere
- $x > 0$  : right hemisphere

The notes of the neurons in the right hemisphere is doubled (one oct. higher) when *Hemisphere mode* is enabled.

The user can either choose to include one hemisphere or both.

**$\mathbf{F_d}(n)$**  The current value of the fluorescence signal is scale according to the normalized size of the corresponding ROI's bounding box. The normalized size  $size_{i_N}$  is obtained with the relation

$$size_{i_N} = \frac{size_i}{size_{max}} \quad (9)$$

Where  $size_i$  is the size in pixel of the corresponding ROI, and  $size_{max}$  is the size of the largest ROI. This coefficient is scaled with interpolating curve, multiplied with  $\mathbf{F_d}(n)_i$  and fed to the poly object.

##### 3.1.2 inside poly

After entering the poly object, the fluorescence goes through a DC removing filter and a digital waveguide, then is fed to the operator.

**DC remover** The DC remover is intended to remove static component in the fluorescence, which tends to be hear tiring and less significant. It is implemented with the Gen object dcblock<sup>4</sup>.

**Waveguide** The driving fluorescence then goes through a karplus-strong waveguide that is intended to mimic a plucked string, in order to add oscilation to the amplitude of the activated ROIs. Its schematic is pictured figure .

The left side, the "neck" (resp. "bridge") is associated with the delay  $N_n$  (resp.  $N_b$  and the reflection  $r_n$  (resp.  $r_b$ ). The position  $pos \in [0, 1]$  represents the position of plucking.

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<sup>4</sup> $y(n+1) = x(n) - x(n-1) + 0.09997y(n-1)$

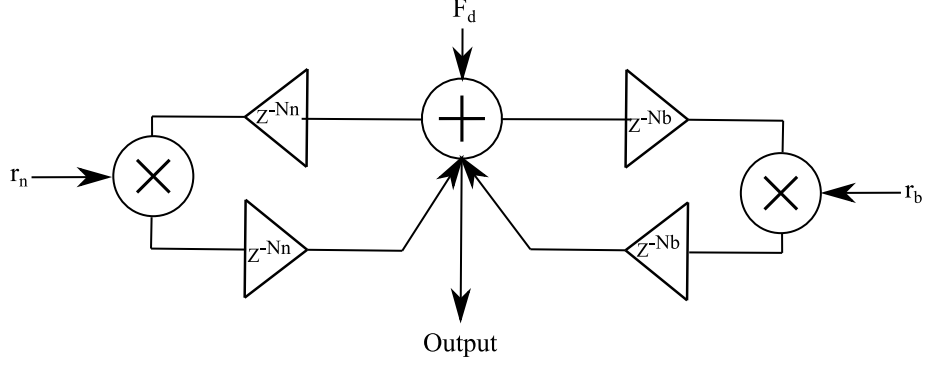


Figure 2: Implementation of the karplus-strong waveguide.

Therefore, in order to guarantee the stability of the system,  $r_n$  and  $r_b$  have to be chosen so that

$$|r_{n,b}| < 1 \quad (10)$$

Let  $N$  be delay, in samples, corresponding to the full length of the waveguide. The delays  $N_{n,b}$  can be obtained with the relations

$$N_n = (1 - pos) \cdot N/2 \quad (11)$$

$$N_b = pos \cdot N/2 \quad (12)$$

**AM modulation** As of 16/04 an AM modulation is added after the operator (described in the following) for aesthetic purpose. The outcoming signal  $s_{out}$  is written as

$$s_{out} = s_{in} (1 - k + k) \sin(2\pi a f t) \quad (13)$$

Where  $f$  is the note of the corresponding poly,  $k$  is the modulation depth and  $a$  an arbitrary coefficient. As of writing it is unclear whether the parameters will be accessible to the user.

**comb filter** As of 16/04 a comb filter (genExpr examples implementation) is added before the panning for aesthetic purpose. Its parameters (feedback/feedforward coefficients, delay and gain) are accessible to the user, given the various results one can obtain.

**Panning** The sources are distributed according to the position of the neuron along the  $x$  axis, a negative value being at the left, a positive value at the right and the origin at the center.

### 3.2 Structure of a single operator<sup>5</sup>

The driving parameters are fed to FM operators, the output is panned with the position of the neuron on the video (position of the centroid of the bounding rectangle). A lowpass filter and a waveshaping buffer are implemented after the synthesis, but not used at the moment of writing. The neurons are equalized using an isotonic curve.

### 3.3 Group Parameter computation<sup>6</sup>

**Computation** The group parameter is computed at each frame. In order to do so, the components of  $\mathbf{F}_n(n)$  or  $\frac{d\mathbf{F}_n(n)}{dt}$  are grouped by clusters for computation. Four group parameters are currently implemented : *Average*, *Average first derivative*, *activation ratio*, and *activation ratio*

<sup>5</sup>poly

<sup>6</sup>synthesis/comp\_group\_parameters

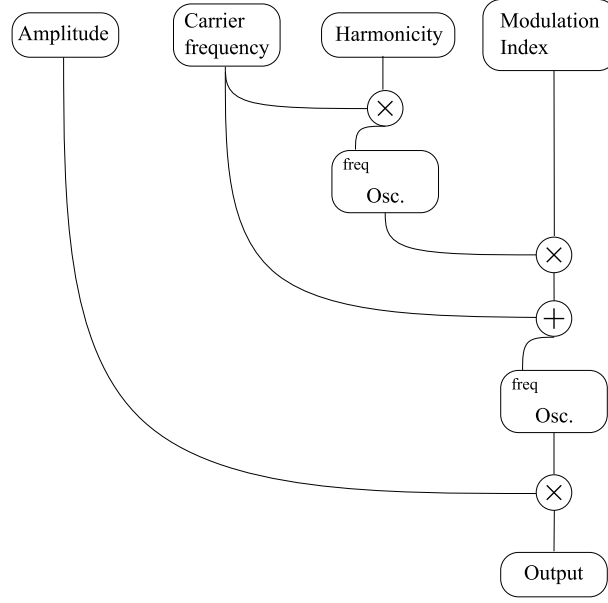


Figure 3: structure of a single operator. Both oscillator uses a sinus wavetable. Harmonicity is currently set to 1.

*first derivative*. In the following  $N_g$  designates the number of neurons in the cluster  $g$ ,  $\mathbf{F}_{\mathbf{n}}(n)_g$  (resp.  $\frac{d\mathbf{F}_{\mathbf{n}}(n)}{dt}$ ) designates the signals (resp. first derivative of the signal) associated with the neurons belonging to the cluster  $g$ . For the sake of simplicity, in the following we only consider the use of the fluorescence, but the expressions are equivalent when using  $\frac{d\mathbf{F}_{\mathbf{n}}(n)}{dt}$ .

- Average :  $\frac{\sum_g \mathbf{F}_{\mathbf{n}}(n)_g}{N_g}$ , where  $\sum_g$  designates the summation over the whole group  $g$ .
- Activation ratio :  $\frac{\sum_g \mathbf{F}_{\mathbf{n}}(n)_{g,>0}}{N_g}$  where  $f_{n_{g,>0}} = 1$  if  $\mathbf{F}_{\mathbf{n}}(n)_g > 0$ , 0 otherwise.

The derivative of the above is computed using a backward finite difference scheme ( $o(h)$ ).

**Scaling** <sup>7</sup> The computed parameter is scaled using two interpolating curves. One scale the parameter itself, the other scales the modulation Index. The scaled output is amplified by a factor set by the user in order to control the range of variation.

## 4 Video, interface and interaction

### 4.1 Playback control<sup>8</sup>

The playback is controlled by a counter which goes from 1 to the number of frames. The user can jump to a frame by clicking on the interface. The playing rate (i.e. the time step and the control rate) can be changed.

### 4.2 Overlay, neuron selection and allocation<sup>9</sup>

The neuron are represented by the bounding boxes of their ROIs. Thus, the user can select them by clicking on the video. A schematic of the bound boxes is presented figure 4.2.

<sup>7</sup>Mapping panel

<sup>8</sup>ui

<sup>9</sup>video/overlay, settings/interaction

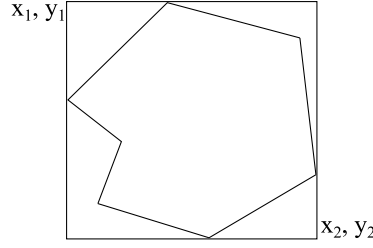


Figure 4: schematic of a bounding box and the associated ROI. The rectangle is represented by its top left and bottom right corners.

Therefore when the mouse is clicked at the point  $x_s, y_s$ , the selected neuron is so that  $x_1 < x_s < x_2$  and  $y_2 < y_s < y_1$ . When a cluster has been selected by the user, the neuron is allocated to the cluster and the overlay is updated.

The overlay displays the centroid of the bounding boxes along with the colors which represent the clusters. It is drawn at initialization and when it has to be updated.

### 4.3 *graphs*<sup>10</sup>

The `graph.maxpat` patcher is implemented to allow the user to track the activity in a single neuron. The plotted data is the normalized fluorescence  $\mathbf{F}_n(n)$ . When the button Set is clicked, a gate opens to let the mouse position in, in order for the user to select a neuron.

At each frame,  $\mathbf{F}_n(n)$  is fed to the patcher which picks up the value corresponding to the selected neuron and plots it.

The tracked neurons are stored in a coll. and displayed in a dedicated overlay<sup>11</sup>. Another overlay displays a blinking dot to remind the user which neuron corresponds to the graph<sup>12</sup>. The group tracking patcher works on the same principle.

## 5 implemented but not used

A waveshaping buffer is implemented. For instance it is filled with the identity. I have tried several functions (mainly  $x^k$  for different  $k$ ), in order to expand the variation between low activation and high activation, but the main result was a sharper sound.

A compressor is implemented in the synthesis, but it is barely compressing, and in my opinion is not that useful.

## 6 Initialization sequence

The initialization process is launched in the subbatch *Init*.

1 data

- loads Clusters
- loads Rois
- \* compute the number of ROIs
- loads raw data
- loads notes
- load initial gains

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<sup>10</sup>`graph.maxpat`

<sup>11</sup>`video/overlay`

<sup>12</sup>`video/overlay`

## 2 processing

- initialize the number of neurons inside the group for the preprocessing *average*
- Launch *average* preprocessing

## 3 normalization

- Set to *bypass*
- write the normalized data collection
- Computes the means and standard deviation vectors

## 4 videoplane

- load video
- get number of frames, dimension of the video
- initialize the counter with the number of frames

## 5 world

- disable the window resizing by the user
- enable the mouse tracking
- start video rendering

## 6 overlay

- get movie dimensions
- get video dimensions
- compute the centers of the ROIs
- display the ROIs

## 7 synthesis

## 8 ui

## 9 Buffers

## 10 selected group