

EEG – GAN :

Generative adversarial networks for electroencephalographic(EEG) brain signals

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- Introduce **modification** to the improved training of **Wasserstein GANs**(WGAN-GP) to stabilize training
 - Also, investigate a range of architectural choices critical for time series generation
- For evaluation,
 - Inception score
 - Frechet inception distance
 - Sliced Wasserstein distance
 - Euclidean distance
- It thus opens up a range of new generative scenarios in the neuroscientific and neurological context
 - Data augmentation of a certain class
 - EEG restoration

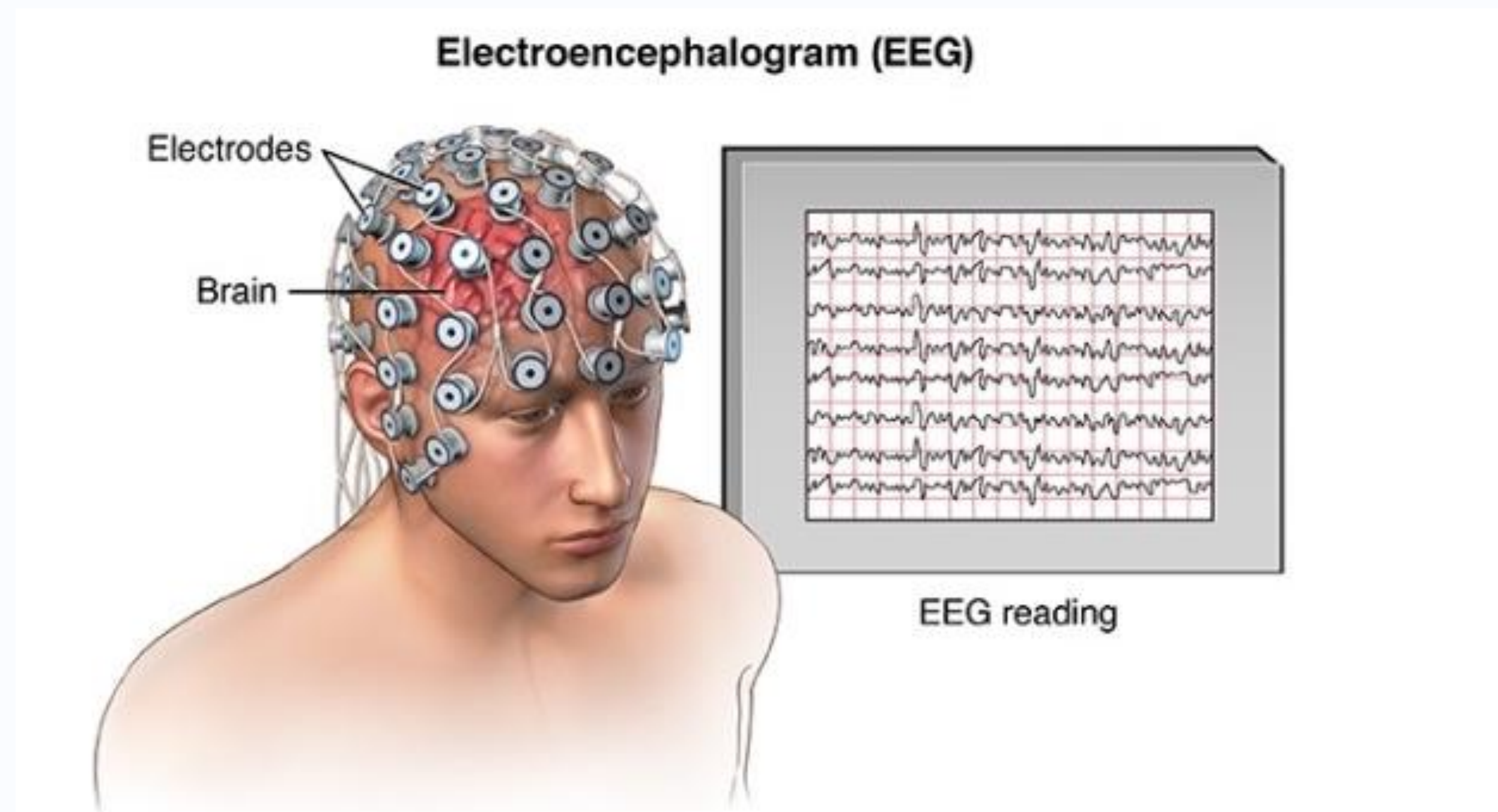
Introduction

- Vanilla GANs suffered heavily from training instability and were restricted to low resolution images.
- GANs have mainly been developed and applied to the generation of images and only a few studies investigating time series were conducted.
- No research regarding the generation of raw EEG signals with GANs has been published at this time.
- To generate naturalistic samples of EEG data, we **propose** an **improvement** to the **Wasserstein GAN** training showing increased training stability.

Data

EEG data

- **128 – electrode EEG system**
 - Sampling rate = 250Hz
 - Channel FCC4h (range = alpha, beta, high gamma)
 - Use Single channel ‘ FCC 4h ‘
 - Overall dataset = 438 signals
 - Training data = 286, validation = 72, test 80

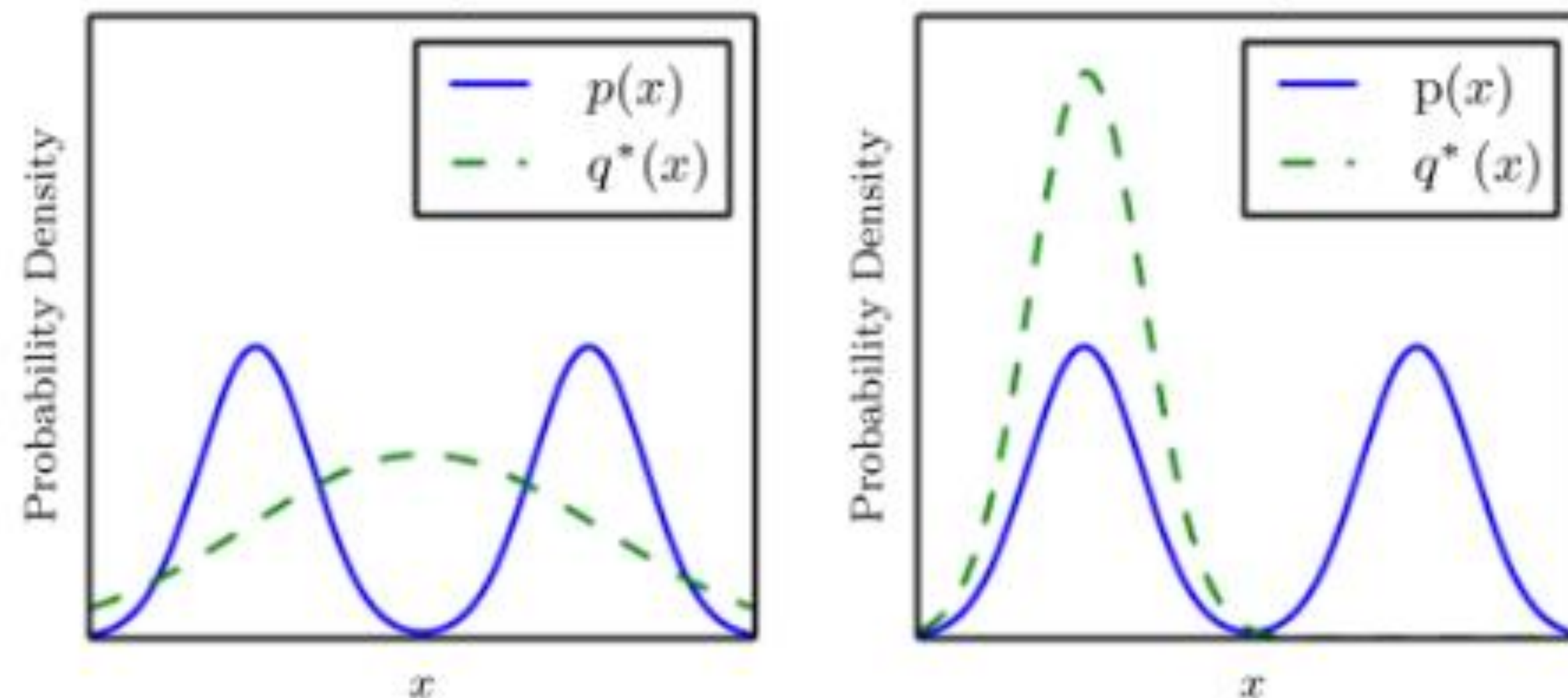


Method

GAN background and improvement

- Vanilla GAN's draw back

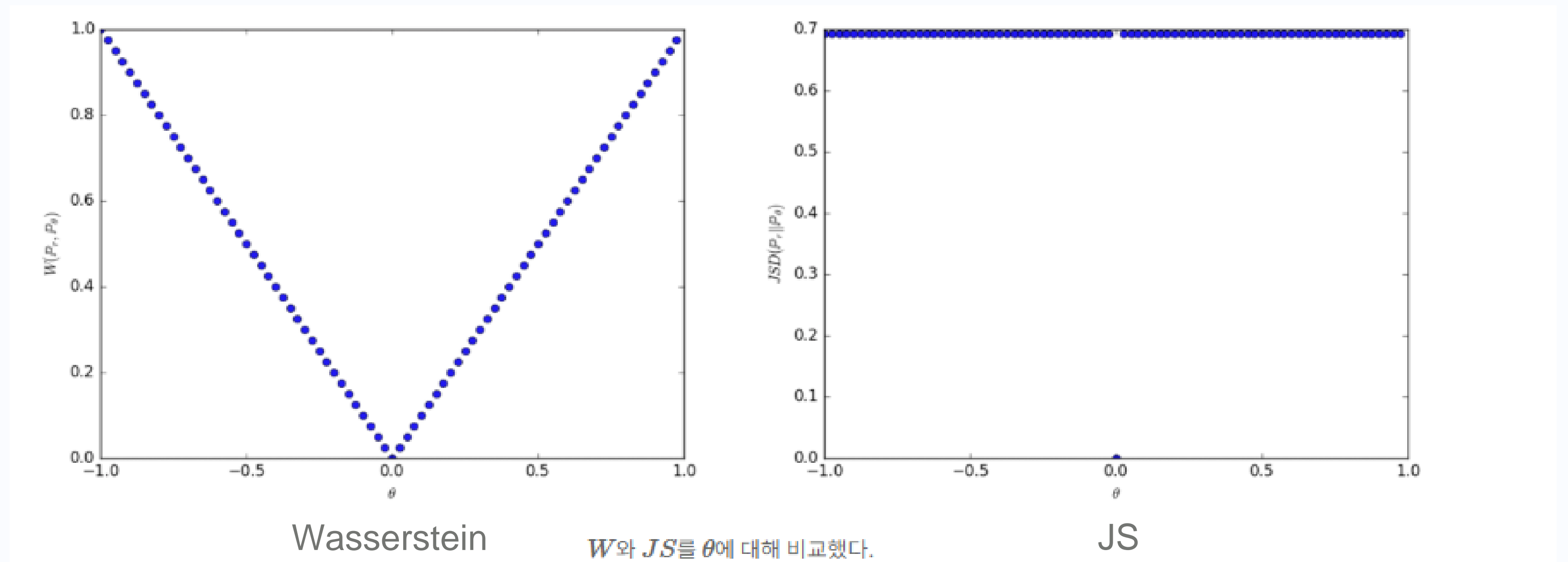
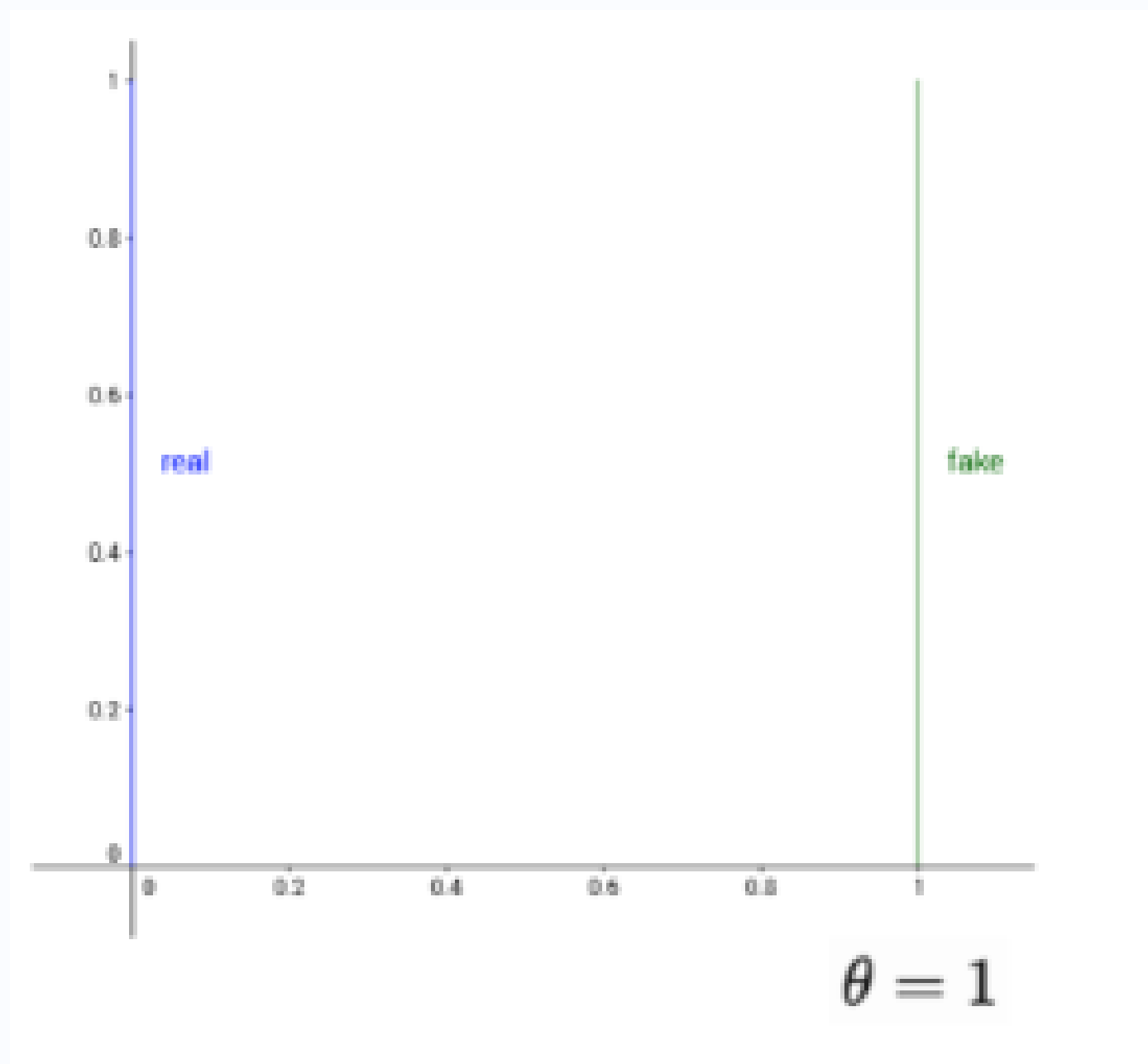
- Vanilla GAN framework tries to minimize the Jensen-Shannon (JS) divergence between the real data distribution P_r and fake data distribution P_f
- If the discriminator is trained to optimality this may lead to the problem of vanishing gradients for the generator. (Problem)
- Mode collapsing problem



Method

WGAN

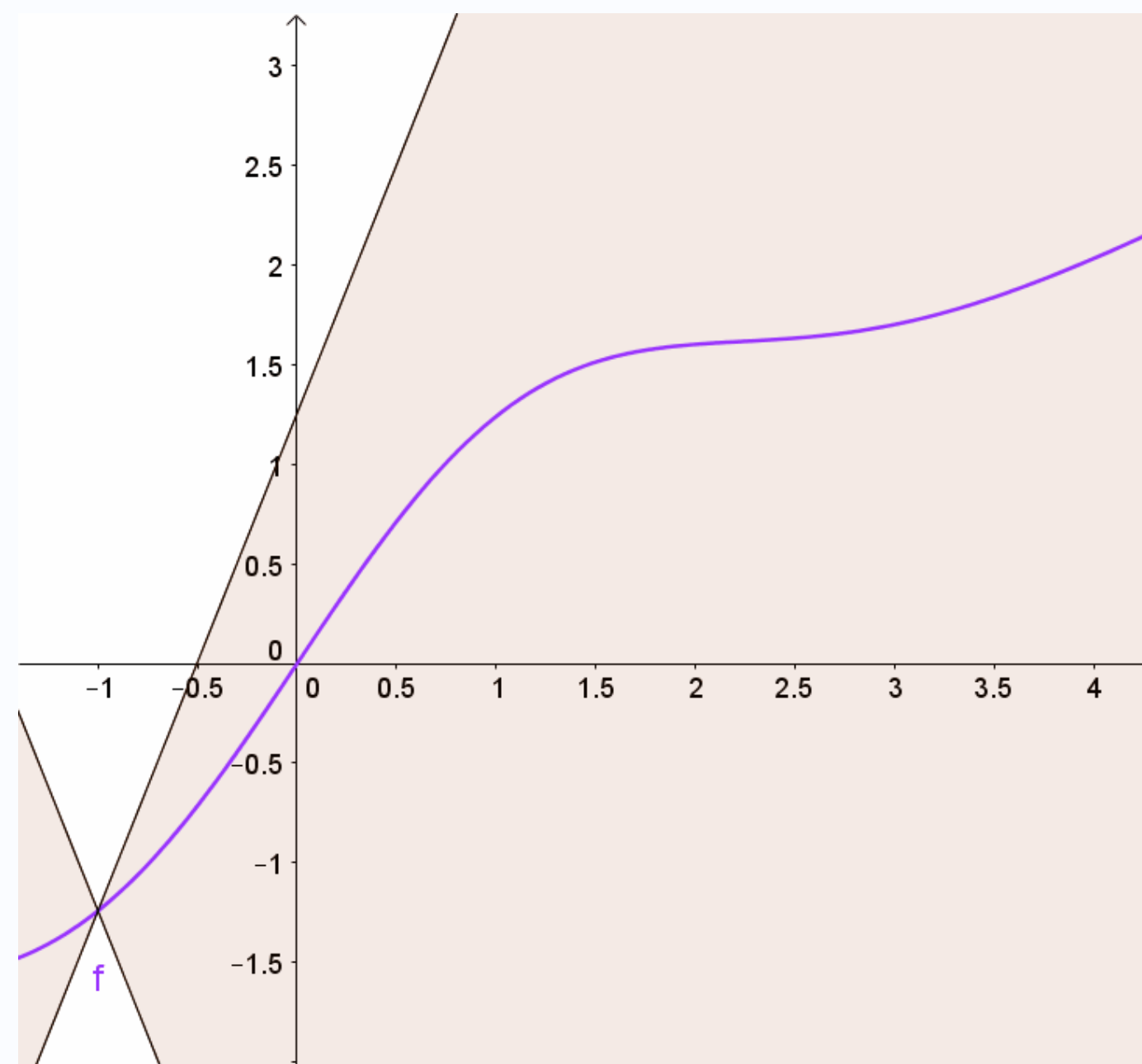
- **Wasserstein GAN** shows training stability.
- WGAN use wasserstein distance while GAN use Jensen-Shannon divergence.



Method

WGAN - Clipping

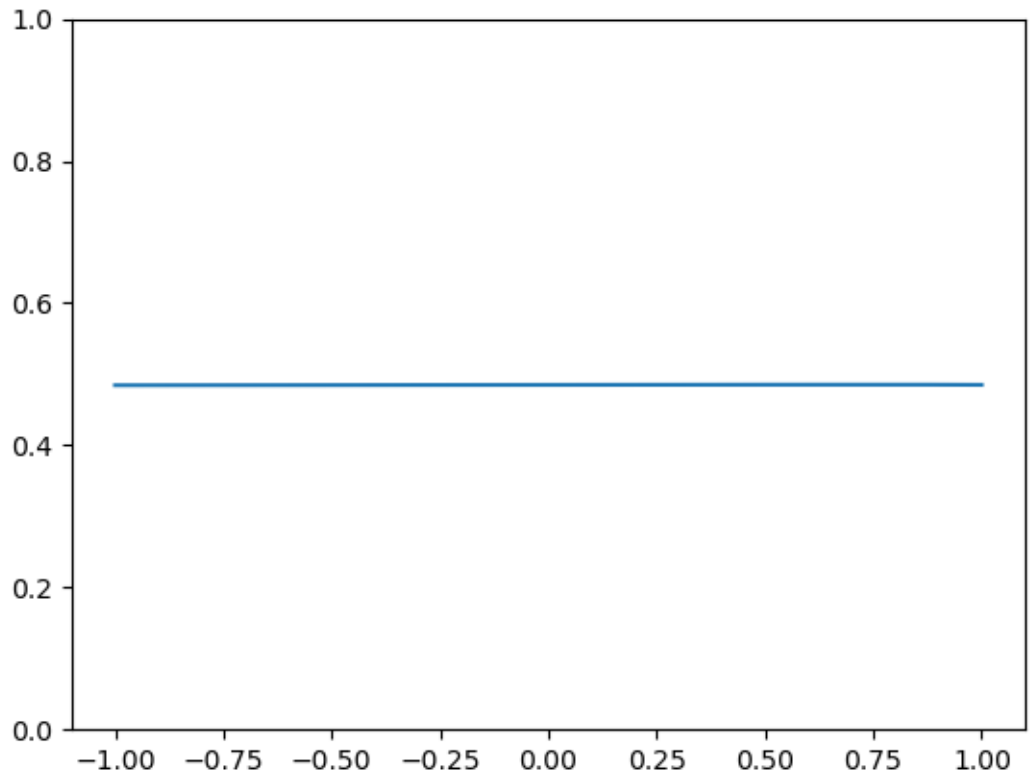
- WGAN enforce **Lipschitz continuity** ($\|f\|_L \leq k$) by clipping the weights of the discriminator to interval $[-c, c]$
- Limiting weights , however, leads to an undesired convergence(vanishing or exploding) of network parameters to those limits.



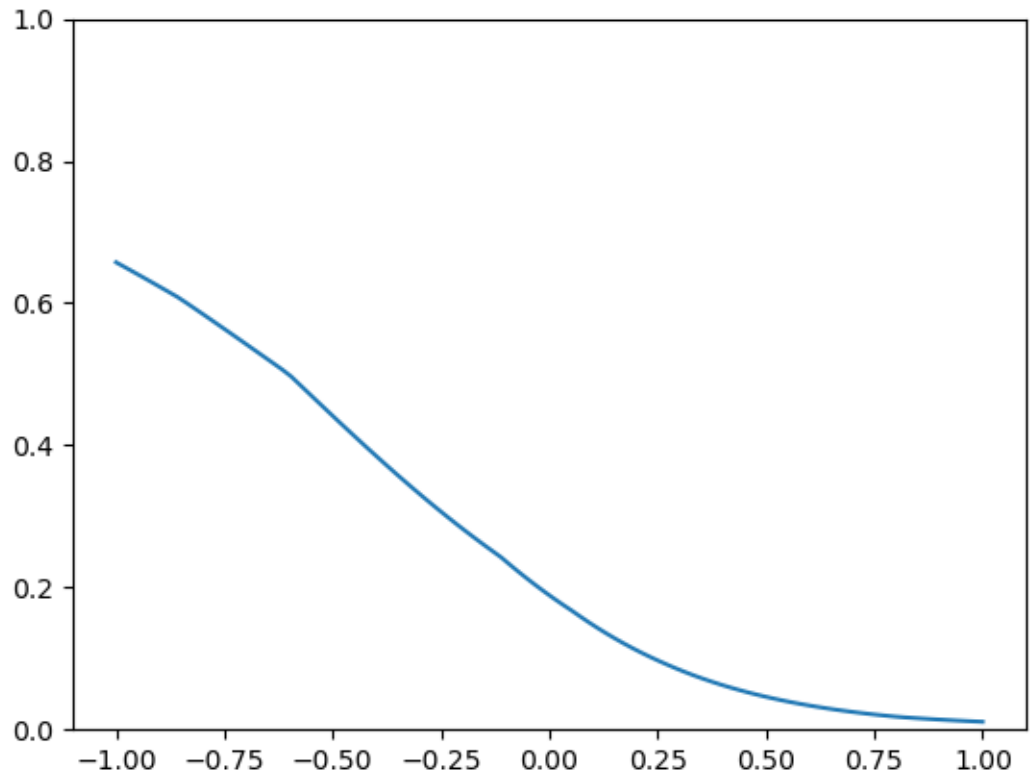
$$|f(x_1) - f(x_2)| \leq k|x_1 - x_2|, k \geq 0 \rightarrow f \text{ enforce K-Lipschitz continuous}$$

Method

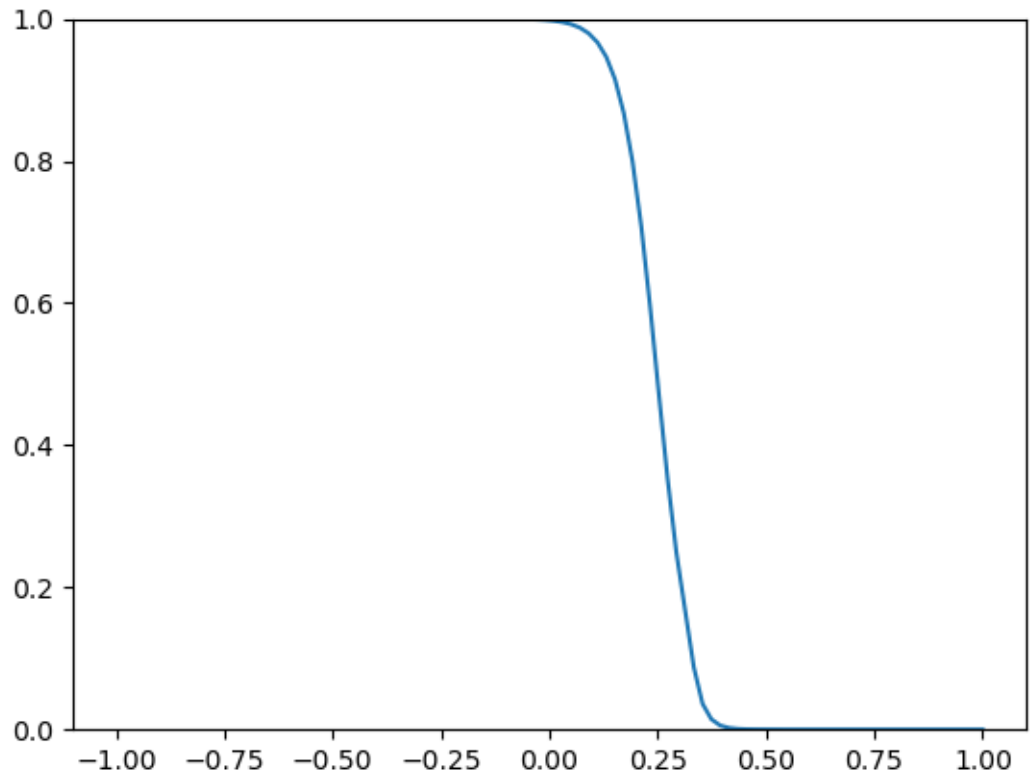
WGAN - Clipping



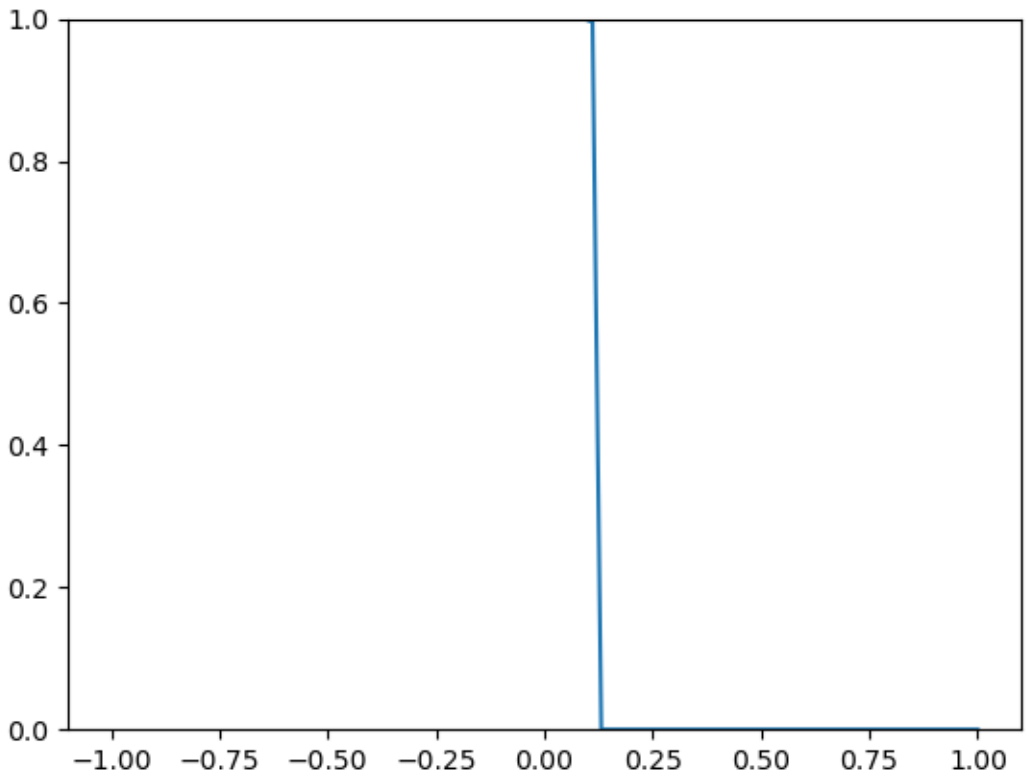
$C = \{-0.1, 0.1\}$



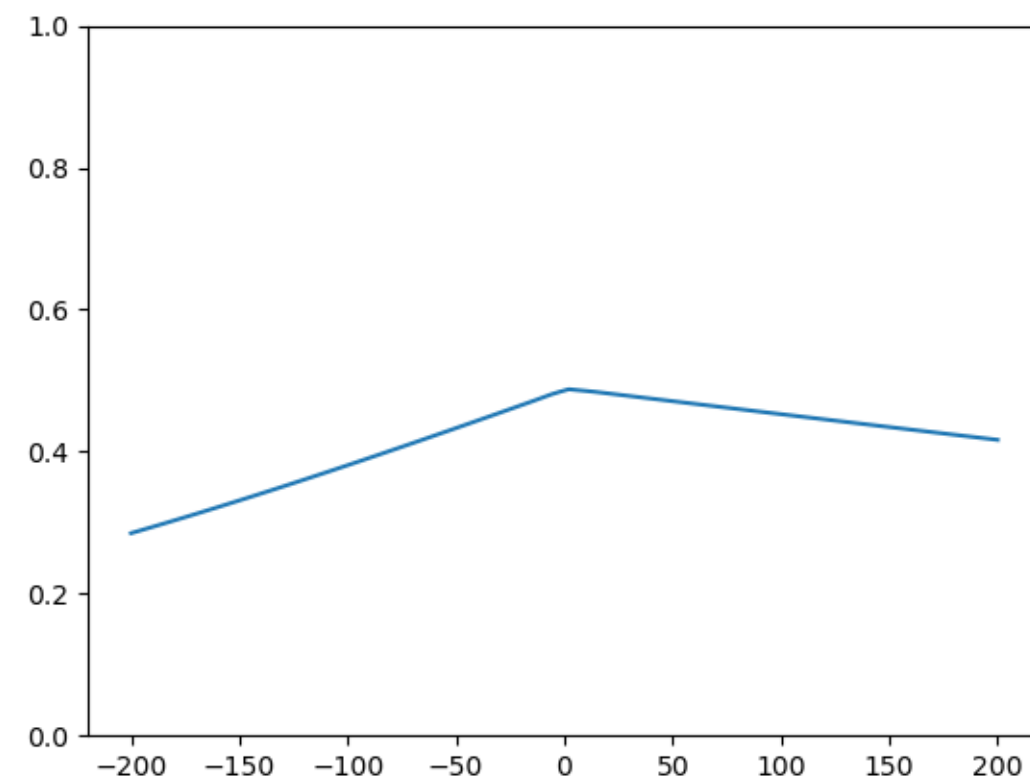
$C = \{-1, 1\}$



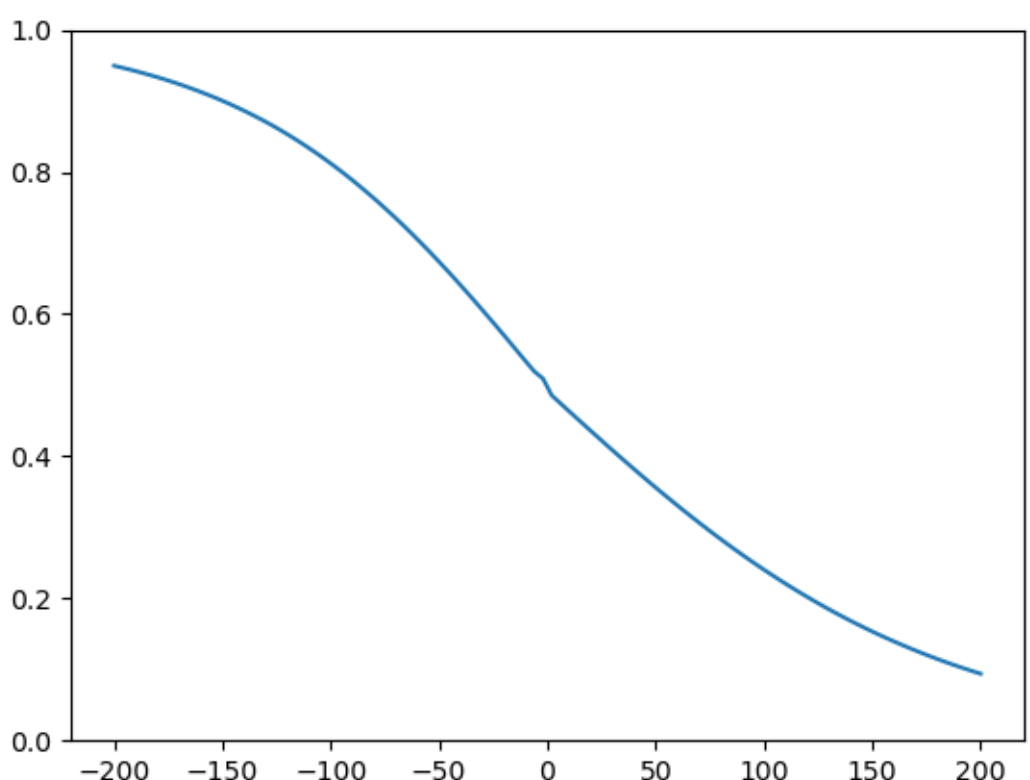
$C = \{-5, 5\}$



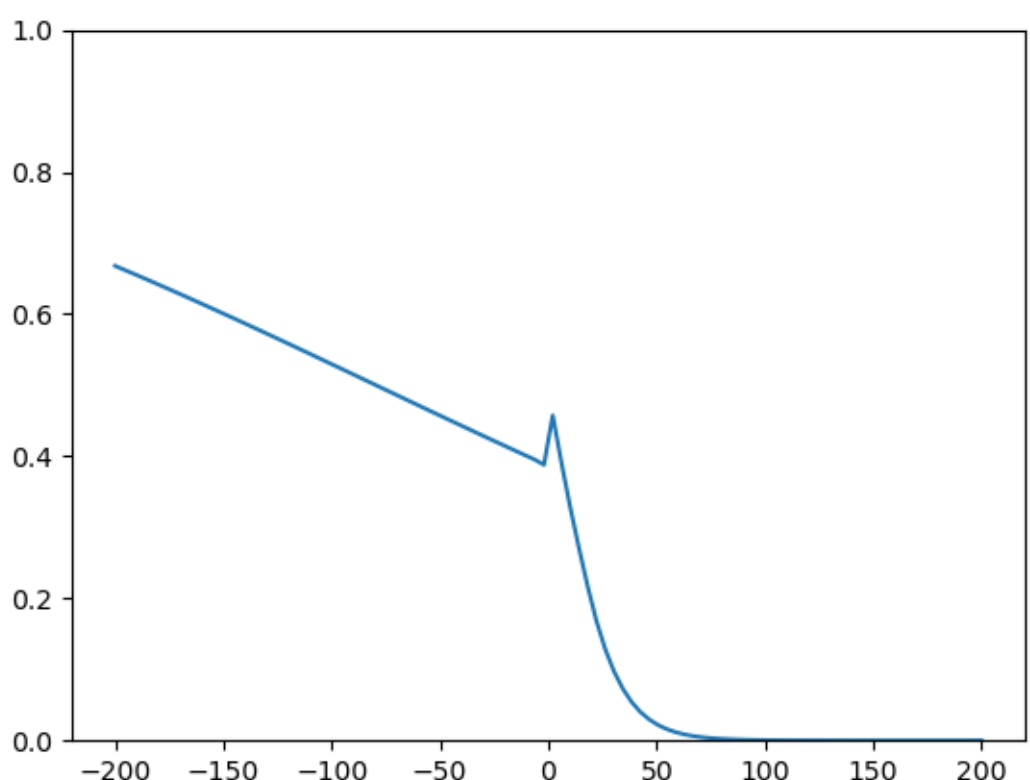
$C = \{-50, 50\}$



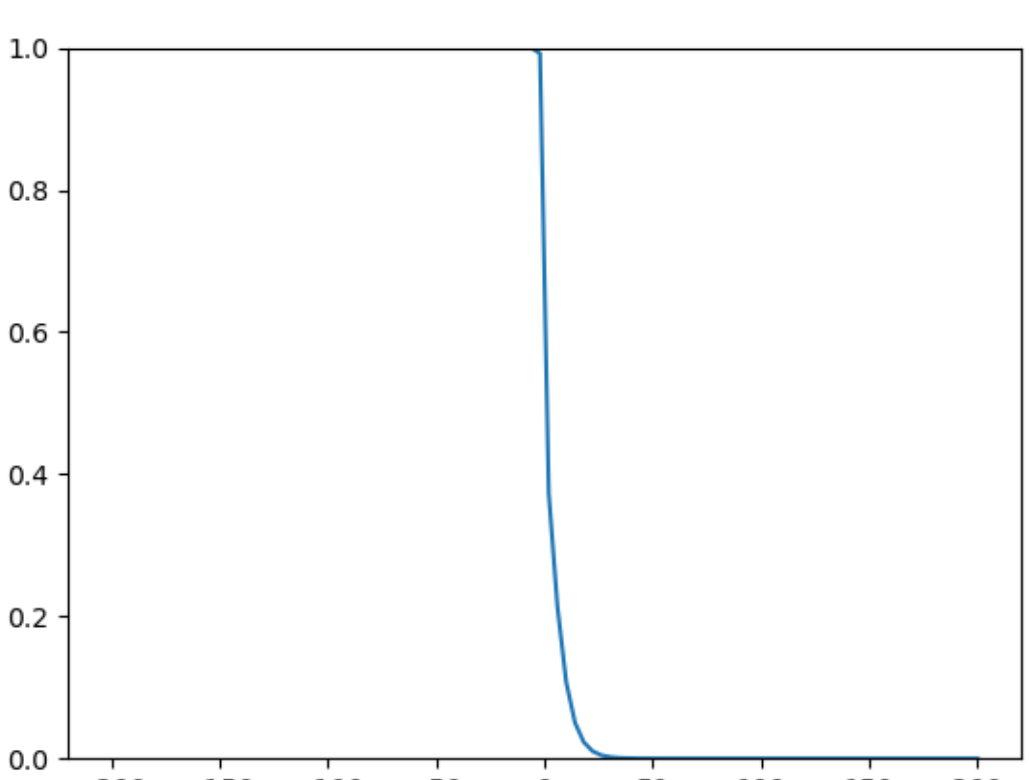
$C = \{-0.1, 0.1\}$



$C = \{-0.2, 0.2\}$



$C = \{-0.5, 0.5\}$

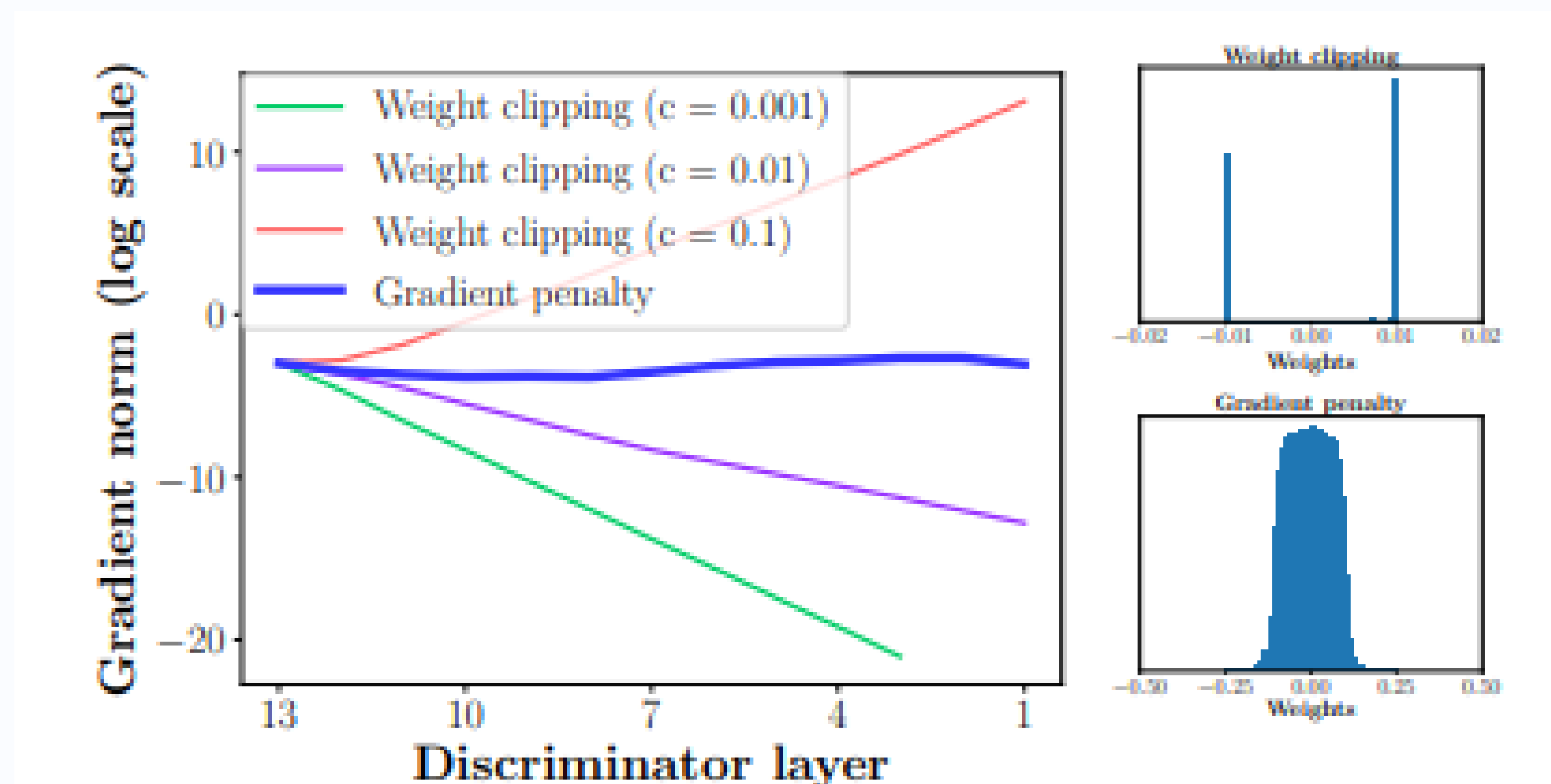


$C = \{-1, 1\}$

Method

WGAN - clipping

- **WGAN** optimization process is difficult because of interactions between the weight constraint and the cost function, which result in either vanishing or exploding gradients without careful tuning of the clipping threshold c .



Method

Clipping -> GP

- Propose an alternative way to enforce the **Lipschitz constraint**.
- We consider directly constraining the gradient norm of the critic's output with respect to its input.
- WGAN GP (Gradient Penalty) gives gradient penalty in loss.

$$L_{P_2} = \underbrace{E_{\tilde{x} \sim P_g}[D(\tilde{x})] - E_{\tilde{x} \sim P_r}[D(x)]}_{\text{Original critic loss}} + \underbrace{\lambda E_{\tilde{x} \sim P_{\tilde{x}}}[(\|\nabla_{\tilde{x}} D(\tilde{x})\| - 1)^2]}_{\text{Gradient penalty}}$$

$$P_1 = \lambda E_{\tilde{x} \sim P_{\tilde{x}}}[\max(0, \|\nabla_{\tilde{x}} D(\tilde{x})\| - 1)^2]$$

$$P_2 = \lambda E_{\tilde{x} \sim P_{\tilde{x}}}[(\|\nabla_{\tilde{x}} D(\tilde{x})\| - 1)^2]$$

Method

Proposed method

- We will not use the two-sided penalty P2
- They did not state a specific reason to choose the two-sided penalty over the one-sided penalty, but preferred it from empirical results.
- The resulting loss function for the critic Generative adversarial networks for brain signals then becomes: **Proposed Loss function**
- Instead of only weighting the penalty term with λ , we also scale it by the current critic difference

$$\widetilde{W}(P_r, P_{theta})$$

$$L_c = E_{\tilde{x} \sim P_{theta}}[D(\tilde{x})] - E_{\tilde{x} \sim P_r}[D(x)] + \max(0, \widetilde{W}(P_r, P_{theta}) \cdot P_1)$$

$$- \widetilde{W}$$

Training and architecture choices

Network architecture

- We start at a resolution 24 time samples and increase the resolution by factor **2** over **6** steps to arrive at 768 samples.
- Factor 2 introduced the least frequency artifacts and led to the best results.
- Use Upsampling : cubic interpolation, linear interpolation, nearest-neighbor upsampling
 - NN upsampling introduces strong high-frequency artifacts
 - CUB, LIN lead to much weaker artifacts

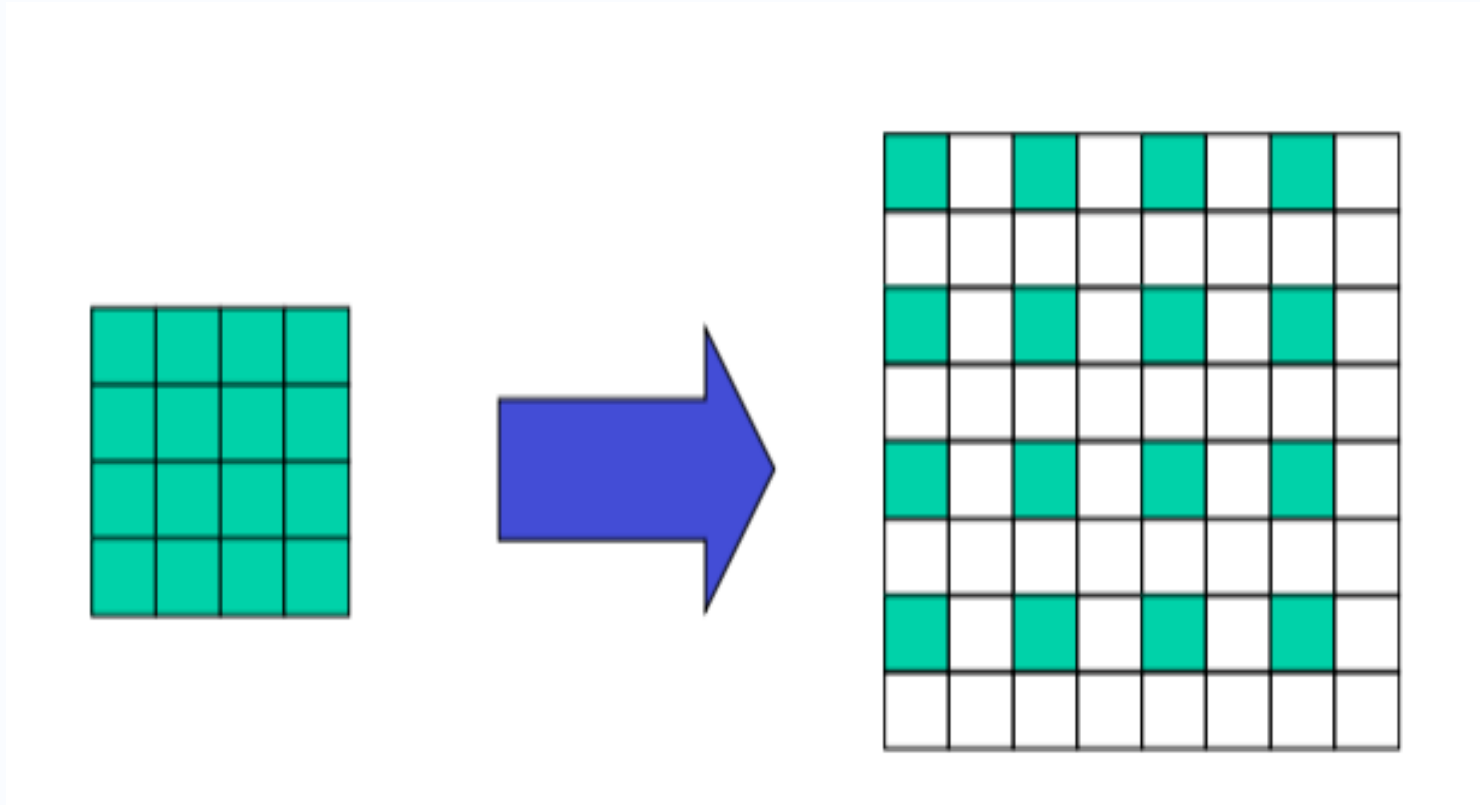
Table 1. Network architecture

(a) Generator			(b) Critic		
Layer	Act./Norm.	Output shape	Layer	Act.	Output shape
Latent vector	-	200 x 1	Input signal	-	1 x 768
Linear	LReLU	50 x 12	Conv 1	LReLU	50 x 768
Upsample	-	50 x 24	Conv 9	LReLU	50 x 768
Conv 9	LReLU/PN	50 x 24	Conv 9	LReLU	50 x 768
Conv 9	LReLU/PN	50 x 24	Downsample	-	50 x 384
Upsample	-	50 x 48	Conv 9	LReLU	50 x 384
Conv 9	LReLU/PN	50 x 48	Conv 9	LReLU	50 x 384
Conv 9	LReLU/PN	50 x 48	Downsample	-	50 x 192
Upsample	-	50 x 96	Conv 9	LReLU	50 x 192
Conv 9	LReLU/PN	50 x 96	Conv 9	LReLU	50 x 192
Conv 9	LReLU/PN	50 x 96	Downsample	-	50 x 96
Upsample	-	50 x 192	Conv 9	LReLU	50 x 96
Conv 9	LReLU/PN	50 x 192	Conv 9	LReLU	50 x 96
Conv 9	LReLU/PN	50 x 192	Downsample	-	50 x 48
Upsample	-	50 x 384	Conv 9	LReLU	50 x 48
Conv 9	LReLU/PN	50 x 384	Conv 9	LReLU	50 x 48
Conv 9	LReLU/PN	50 x 384	Downsample	-	50 x 24
Upsample	-	50 x 768	Conv 9	LReLU	50 x 24
Conv 9	LReLU/PN	50 x 768	Conv 9	LReLU	50 x 24
Conv 9	LReLU/PN	50 x 768	Downsample	-	50 x 12
Conv 1	-	1 x 768	Linear	-	1 x 1

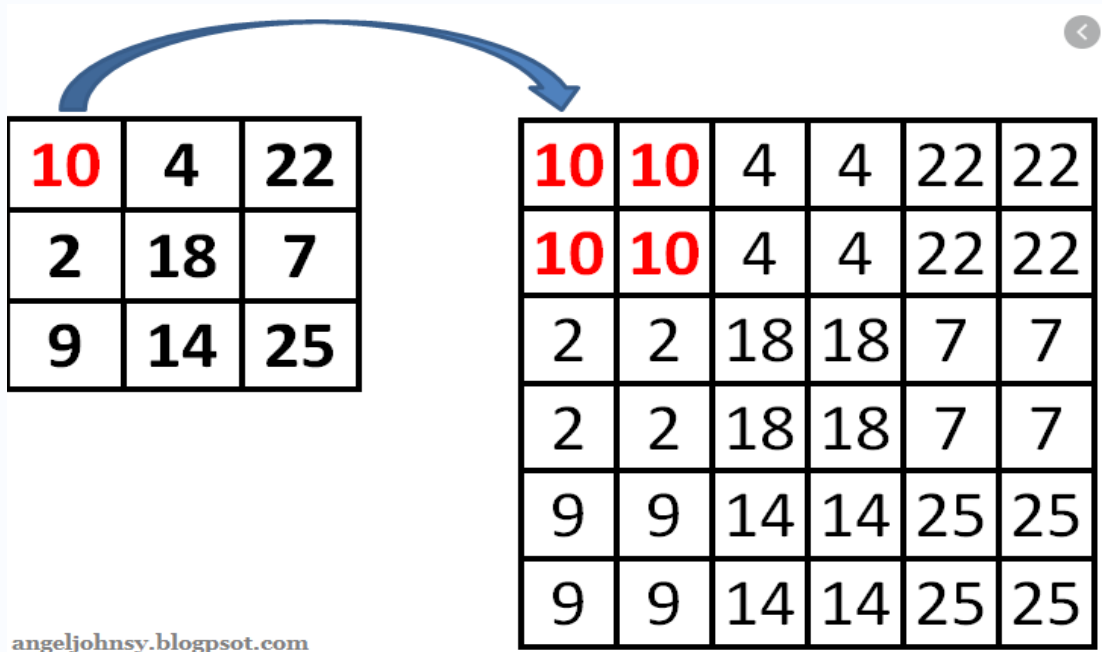
Training and architecture choices

Network architecture

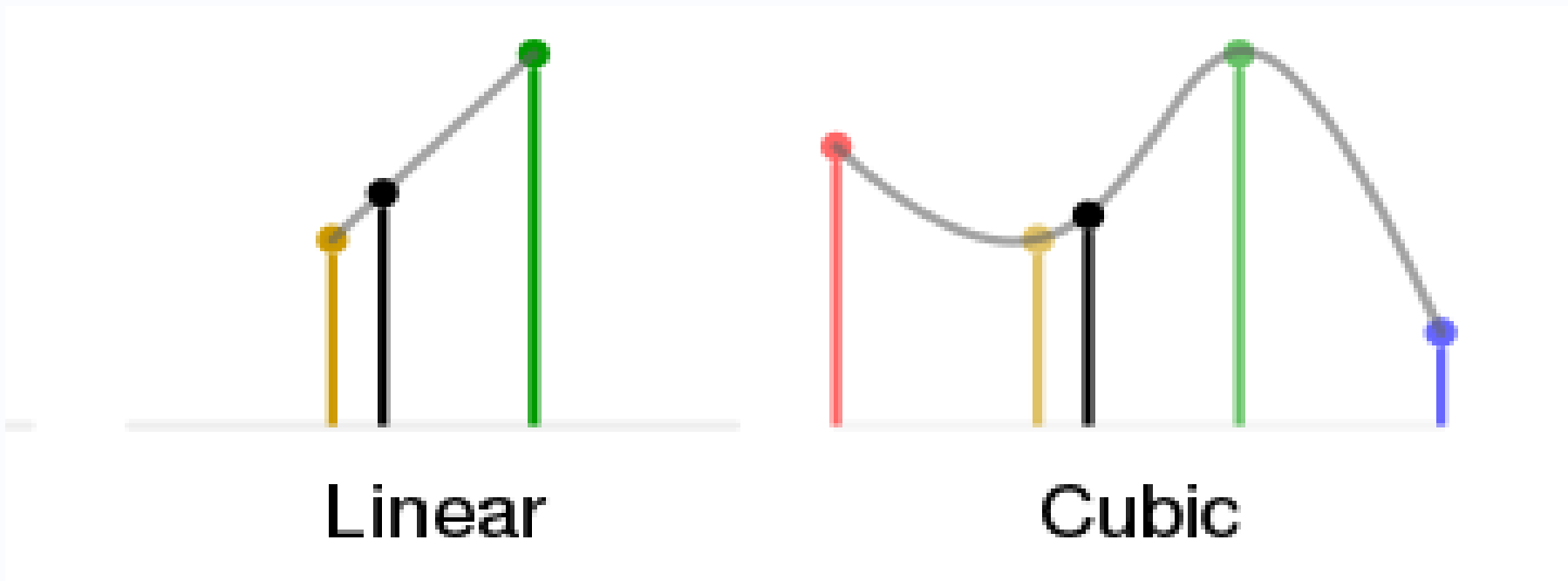
- Upsampling Interpolation



upsampling



NN upsampling

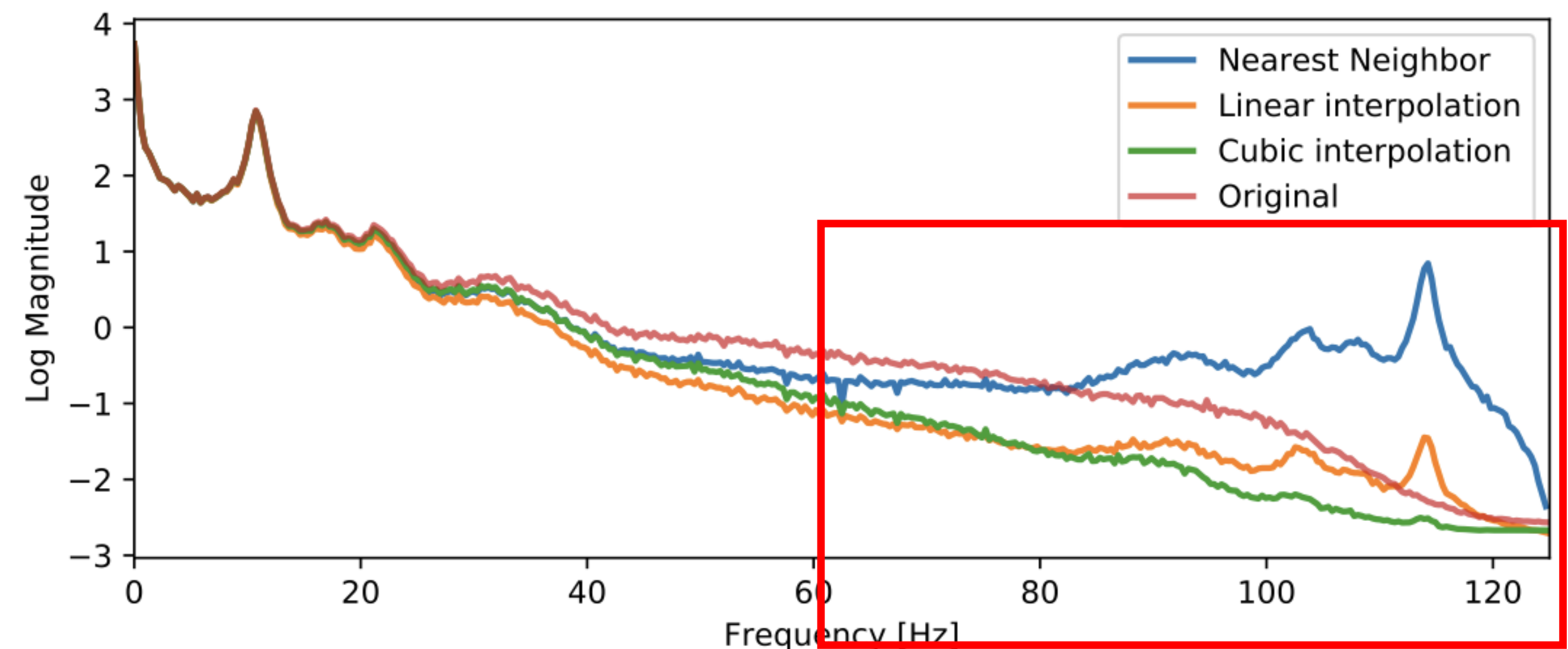


interpolation

Training and architecture choices

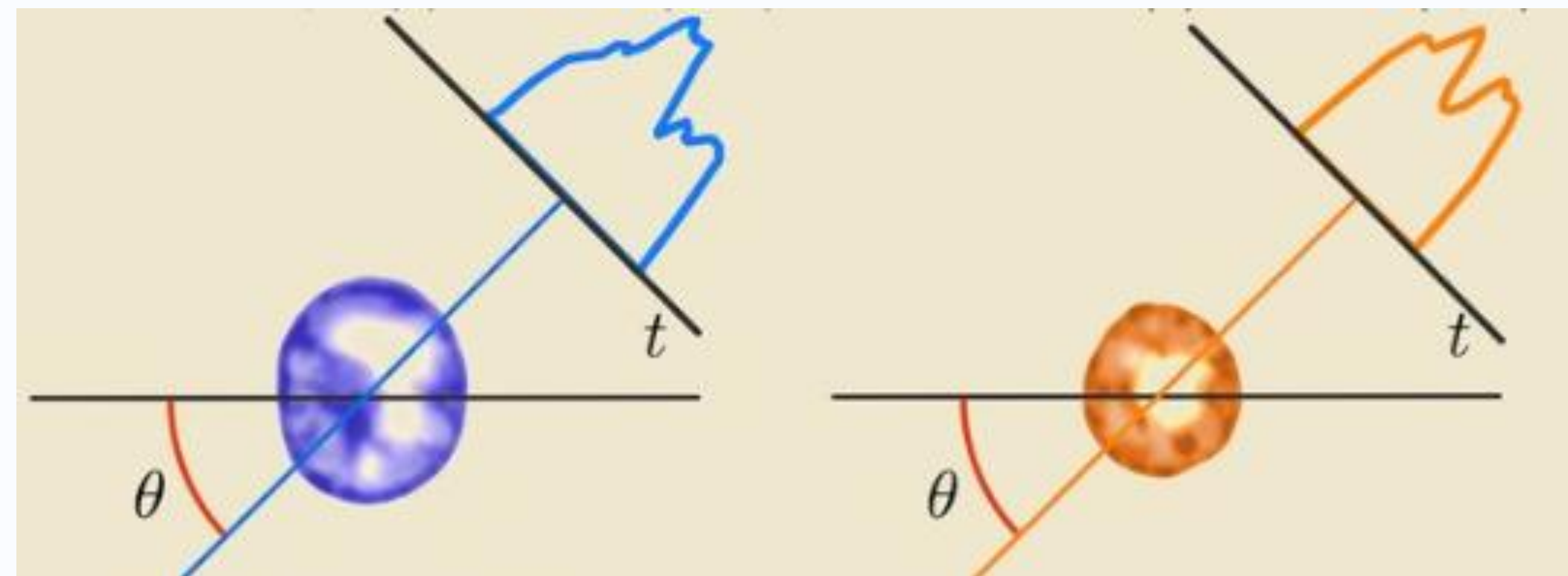
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Evaluation metrics

- INCEPTION SCORE
- FRECHET INCEPTION DISTANCE
 - > real data & fake data feature space distance
 - > $FID^2 = \|m_f - m_r\|^2 + Tr(C_f + C_r - 2(C_f C_r)^{\frac{1}{2}})$
- EUCLIDEAN DISTANCE (??? 왜 마이너스지 ???)
- SLICED WASSERSTEIN DISTANCE



Results

- WGAN-GP model collapsed (IS gave no strong evidence for the collapse of the mode but the others)
- Different architectures performed best for different metrics.

- CONV-LIN performed best for IS
- AVG-NN performed best for FID
- AVG-NN performed best again for ED
- CONV-CUB performed best for SWD

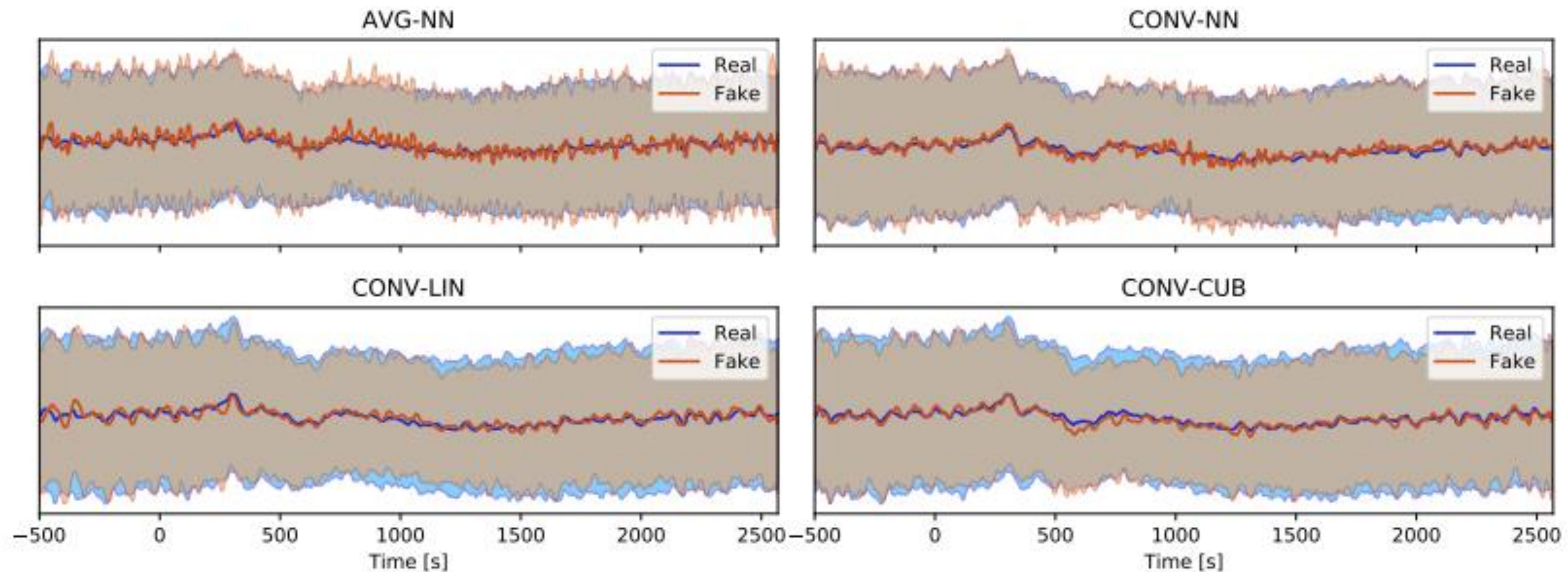
- AVG = average pooling
- NN = nearest-neighbor upsampling
- LIN = linear interpolation
- CUB = cubic interpolation

#	Model	IS	FID	ED _{min}	SWD
1	AVG-NN	1.361	9.523	-0.056	<i>0.102</i>
2	CONV-NN	1.297	16.755	-0.121	0.084
3	CONV-LIN	1.363	11.854	-0.252	0.086
4	CONV-CUB	<i>1.292</i>	<i>33.765</i>	<i>-0.375</i>	0.078
5	WGAN-GP CONV-CUB	1.281	120.854	+0.034	0.309
	Real	1.555	0.	4.653	0.
	Noise	1.049	614.782	+1.061	0.155

Visual inspection

TIME SAMPLES

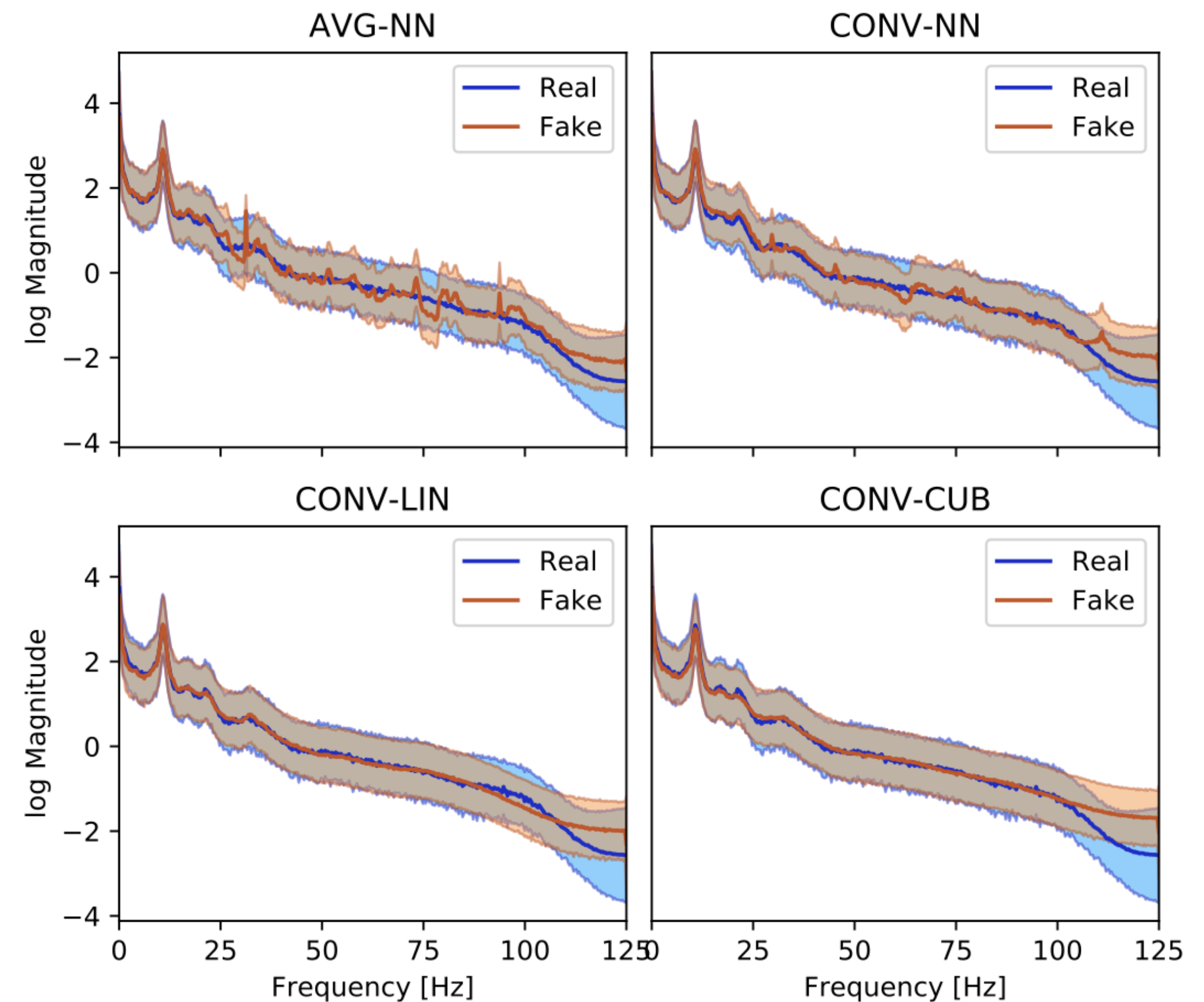
- AVG-NN shows a clear deviation of the generated sample distributions from real data
- CONV-CUB shows a very good fit.



Visual inspection

FREQUENCY SPECTRA

- CONV-LIN and CONV-CUB show a good fit.
- CONV-LIN better fits low frequencies, whereas CONV-LIN shows better fits in high frequencies.
- No model managed to properly fit frequencies higher than 100Hz



Conclusion

- Inception score(IS) did not give meaningful information about the quality of signals generated by a model.
- Also, Frechet inception distances (FID) did not necessarily produce signals with spatial and spectral properties similar to the real input samples.
- The model expressing the most natural looking spatial and spectral distributions had the best sliced Wasserstein distance (SWD).
- Overall, no single metric gave sufficient information about the quality of a model
- Combination of FID, SWD and ED gave a good idea about its possible overall properties

Future works

- Training not only single channel, also multi-channel EEG recordings.
- Understand the impact of different design choices such as convolution size and up-down sampling.

Thank you.