DSP Assignment 2 FIR Filter

Miss Ramon Suwanban (2495594S) Mr Wikara Gunawan (2397833G)

due 9 November 2020 (3PM)

Declaration of Originality and Submission Information

I affirm that this submission is my own / the groups original work in accordance with the University of Glasgow Regulations and the School of Engineering Requirements.

Student Number: 2495594S Student Name: Miss Ramon Suwanban Student Number: 2397833G Student Name: Mr Wikara Gunawan

1 ECG Filtering

1.1 Introduction

Fast Fourier Transform is a transformation which requires the full recording data to perform, so it is not suitable for real-time processing. As a result, the finite-impulse response filter or FIR filter which is a causal digital filter that only takes finite number of sample from the whole data to perform was implemented. However, note that FIR filter only do semi-real time processing because its implementation involves buffer which introduces time delay.

ECG signal measured is subjected to 50 Hz noise and DC line shift which needs to be removed. In cases that almost real time filtering is needed, such as filtering the ECG signal to display on a patient monitor, FIR filter is used instead of Fast Fourier Transform. However, the result from Fast Fourier Transform would actually be more accurate because it takes more sample to process.

FIR filter is written as a function that takes 1 data in and outputs 1 data at a time, so it is used for semi-real time processing. The process of an FIR filter is to sum up the multiplication of the coefficients of the filter and the corresponding data stored in buffer which will be shifted every time a new data is fed. Furthermore, we are using ring buffer to reduce computation resource from normally shifting the array operation.

1.2 Method and Results

The implementation of this part consists of 2 python files, fir_filter.py and ecg_filter.py. fir_filter.py contains the FIR filter class which needs coefficient array as the input. It will automatically runs the **unittest()** if it is run in the **main()** function. ecg_filter.py contains 2 filters made from the FIR filter class(from fir_filter.py) and imports raw ecg data to filter. It saves the results as shortecg.dat(from ECG.dat) and shorteint.dat(from Einthoven_ii Walking).

1.2.1 FIR-filter Function

```
import numpy as np
class FIR_filter:
def __init__(self,coefficients):
self.coeff = coefficients
self.offset = 0
self.buffer = np.zeros(len(coefficients))
```

Listing 1: Initialise Constructor

Import the libraries used by the code.

• numpy: array processing and mathematical calculations

The constructor of the class is initialised with the local variables inside the constructor function: **coeff**, **offset** and **buffer**. **coeff** consists of the input coefficients or the impulse response of the filter. It will be taken from the input

when you instantiate the filter class. **offset** is the position of the current data on the buffer of the processed data which is used only inside the filter class. Finally, **buffer** is created by having an array of zeros with the size of the coefficients number to store all delayed data.

```
def dofilter(self,u):
           result = 0
28
           self.buffer[self.offset] = u
29
           #print("offset index:",self.offset)
30
31
           for i in range(self.offset+1):
               result = result + self.buffer[i]*self.coeff[self.offset
33
      -i]
               #print("buffer index:",i)
34
35
               #print("coeff index:",self.offset-i)
36
           #print("Second For Section")
37
           for i in range(self.offset+1,len(self.buffer),1):
38
               result = result + self.buffer[i]*self.coeff[len(self.
39
      buffer) -1+self.offset+1-i]
               #print("buffer index:",i)
40
               #print("coeff index:",len(self.buffer)-1+self.offset+1-
41
      i)
42
43
           self.offset+=1
           if self.offset>=len(self.buffer):
44
               self.offset=0
46
           return result
47
```

Listing 2: Ring Buffer Function

New input from the outside is put into the **offset** th position of the buffer. Note that the **offset** increments every time a new data was input. It then resets at the maximum size of the length of the buffer, which is the length of the coefficient. There are 2 **for-loop** to operate the multiplication process. The index of the coefficients and the buffer slots multiplied are shown in figure 1.

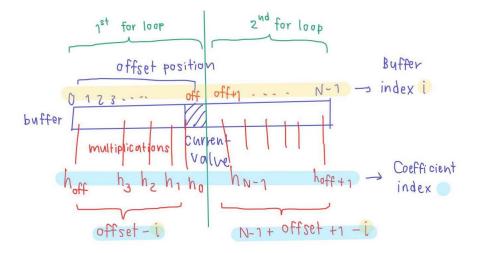


Figure 1: Ring Buffer Index Diagram

dofilterPrint is the exact same function as dofilter, but with the print lines uncommented. We use this dofilterPrint in unittest() only, so we can see which coefficient is being multiplied to which buffer. It also shows which pairs are being done on which for-loop.

```
def dofilterPrint(self,u):
                                        #index printing version for
      diagnosis purpose
          result = 0
51
           self.buffer[self.offset] = u
           print("offset index:",self.offset)
53
54
           for i in range(self.offset+1):
               result = result + self.buffer[i]*self.coeff[self.offset
      -i]
               print("buffer index:",i)
56
57
               print("coeff index:",self.offset-i)
58
           print("Second For Section")
59
60
           for i in range(self.offset+1,len(self.buffer),1):
               result = result + self.buffer[i]*self.coeff[len(self.
61
      buffer) -1+self.offset+1-i]
               print("buffer index:",i)
62
               print("coeff index:",len(self.buffer)-1+self.offset+1-i
64
           self.offset+=1
65
66
           if self.offset>=len(self.buffer):
               self.offset=0
67
68
           return result
69
```

Listing 3: dofilterPrint

unittest() is testing with coefficient [0.5,0.5,0,0] and input [0,1,0,0,0,...](impulse). Because the solution is obvious[0,0.5,0.5,0,0,0,...], it can be used to check primarily if the filter is functioning correctly. The **print** function from the **dofilterPrint** also helps checking the indices.

```
71 def unittest():
          h = np.array([1/2,1/2,0,0,0])
72
          print("Coefficient:",h)
73
74
          f = FIR_filter(h)
          y = f.dofilterPrint(0)
                                       #use the index printing version
75
          print("Input 0, Output",y)
76
          y = f.dofilterPrint(1)
                                       #use the index printing version
77
          print("Input 1, Output",y)
          for i in range (20):
79
              y= f.dofilterPrint(0)
                                       #use the index printing version
              print("Input 0, Output",y)
81
82
83 if __name__ == "__main__":
84 unittest()
```

Listing 4: unittest()

1.2.2 ECGfilter.py

```
import numpy as np
from fir_filter import FIR_filter
from numpy import loadtxt
from matplotlib import pyplot

f s = 250  #Hz
M = 500  #loses 2 heart beat to warm up the filter (2seconds)
```

Listing 5: Import FIR_Filter Class

To initialize the code, fir_filter.py must be located in the same folder, so it could be imported to the code. The sampling frequency is 250 Hz, and the length of the coefficient is 500 elements(number of taps/number of delay buffer). The number of coefficient should be high enough to make frequency resolution becomes enough for the 0.5 Hz frequency cutoff in our DC filter design. Frequency resolution in this case equals 250 Hz / 500 taps = 0.5 Hz which is exactly how good resolution we need. The trade off for high coefficient number is that it takes time for the buffer to fill up before it can actually function.

```
10 # 50 Hz Notch Filter
11 k1 = int(49.5/fs * M)
12 k2 = int(50.5/fs * M)
13
14 Window50 = np.ones(M)
15 Coeff50 = np.ones(M)
16
17 Window50[k1:k2+1] = 0
18 Window50[M-k2:M-k1+1] = 0
19
```

```
20 pyplot.figure(1)
21 pyplot.plot(Window50)
pyplot.title('50 Hz Notch Filter - Ideal')
23 pyplot.xlabel('M (sample number)')
24 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig1.eps', format='eps')
27 W50 = np.fft.ifft(Window50)
28 W50 = np.real(W50)
30 pyplot.figure(2)
31 pyplot.plot(W50)
pyplot.title('50 Hz Notch Filter - IFFT')
33 pyplot.xlabel('Coefficient Index')
34 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig2.eps', format='eps')
37 Coeff50[0:int(M/2)] = W50[int(M/2):M]
38 Coeff50[int(M/2):M] = W50[0:int(M/2)]
39
40 pyplot.figure(3)
41 pyplot.plot(Coeff50)
42 pyplot.title('50 Hz Notch Filter - IFFT(fixed)')
43 pyplot.xlabel('Coefficient Index')
44 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig3.eps', format='eps')
47 Filter50 = FIR_filter(Coeff50)
```

Listing 6: 50 Hz Bandstop Coefficient

To create coefficient array for the 50 Hz removal, an ideal notch filter (sequence of 0s and 1s) is created with targeting of 49.5 Hz ($\mathbf{k1}$) to 50.5 Hz($\mathbf{k2}$) for the cutoff frequencies. The inverse fast-fourier transform is applied to the ideal filter array, then array manipulation is applied to shift the coefficients by half of the length of the coefficient to swap the positions to make it causal and intact.

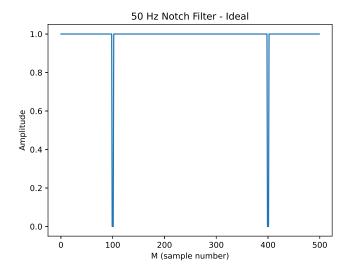


Figure 2: 50 Hz Notch Filter Ideal Frequency Domain Plot

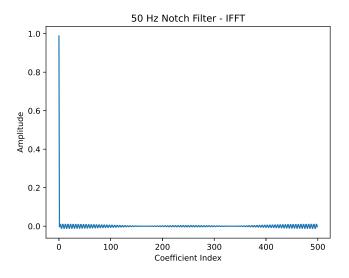


Figure 3: 50 Hz Notch Filter IFFT

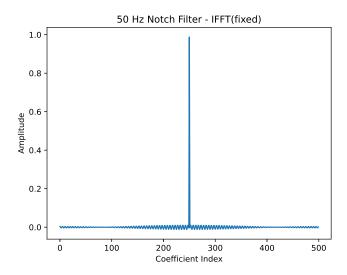


Figure 4: 50 Hz Notch Filter IFFT (fixed) - Coefficients

To remove the DC line shift from the data, a window function coefficient is created by targeting the $0.5~\mathrm{Hz}$ as the cutoff frequency. The same procedure as the $50~\mathrm{Hz}$ notch filter applies.

```
50 #DC filter
51 k3 = int(0.5/fs * M)
52 WindowDC = np.ones(M)
  CoeffDC = np.ones(M)
55 WindowDC[0:k3+1] = 0
56 pyplot.figure(4)
57 pyplot.plot(WindowDC)
58 pyplot.title('DC Filter - Ideal')
59 pyplot.xlabel('M (sample number)')
60 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig4.eps', format='eps')
62
63 WDC = np.fft.ifft(WindowDC)
64 WDC = np.real(WDC)
66 pyplot.figure(5)
67 pyplot.plot(WDC)
68 pyplot.title('DC Filter - IFFT')
pyplot.xlabel('Coefficient Index')
70 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig5.eps', format='eps')
72
73 CoeffDC[0:int(M/2)] = WDC[int(M/2):M]
74 CoeffDC[int(M/2):M] =
                         WDC[0:int(M/2)]
76 pyplot.figure(6)
77 pyplot.plot(CoeffDC)
```

```
78 pyplot.title('DC Filter - IFFT(fixed)')
79 pyplot.xlabel('Coefficient Index')
80 pyplot.ylabel('Amplitude')
81 # pyplot.savefig('ecg_fig6.eps', format='eps')
82
83 FilterDC = FIR_filter(CoeffDC)
```

Listing 7: DC Filter Coefficient

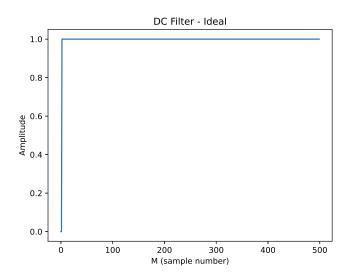


Figure 5: DC Removal Filter Ideal Frequency Domain Plot

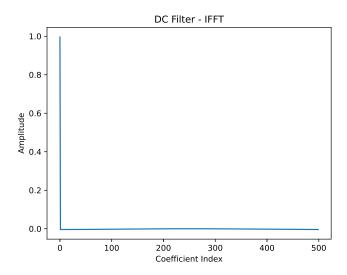


Figure 6: DC Removal Filter IFFT

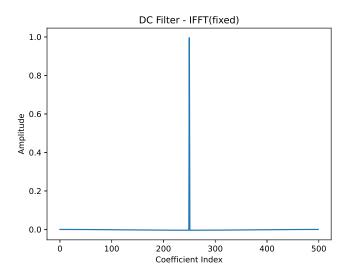


Figure 7: DC Removal Filter IFFT (fixed) - Coefficients

We load .dat ECG data to our file to perform semi-real time processing and plot them in time domain.

```
# load first ECG file
file1 = open('ECG.dat', 'r') #line by line to use as real-time
filter
```

```
91 pyplot.figure(7)
92 print(len(ecg))
93 time = np.linspace(0,len(ecg)/fs,len(ecg))
94 pyplot.plot(time,ecg)
95 pyplot.title('ecg (raw)')
96 pyplot.xlabel('Time(s)')
97 pyplot.ylabel('Amplitude')
98 #pyplot.savefig('ecg_fig7.eps', format='eps')
99
100
101 # Investigate frequency domain
102 fx=np.fft.fft(ecg)
103 fxx = fx/len(ecg)
104 dbs = 20*np.log10(abs(fxx))
                                 # Fourier Transform Normalised
                                # DB Conversion
105 pyplot.figure(8)
freq = np.linspace(0,fs,len(ecg))
pyplot.plot(freq,dbs)
108 pyplot.title('ecg (raw) - Frequency Domain')
pyplot.xlabel('Frequency (Hz)')
pyplot.ylabel('Amplitude')
#pyplot.savefig('ecg_fig8.eps', format='eps')
112
113 #load second ECG data
''', Initialise experiments from the files of einthoven'',
subject_number = 3
116 experiment = 'walking'
117 ecg_class = GUDb(subject_number, experiment)
'','Initialise experiments from the files of einthoven'',
chest_strap_V2_V1 = ecg_class.cs_V2_V1
einthoven_ii = ecg_class.einthoven_II
122
'', Filtered Data With Einthoven',
124 ecg_class.filter_data()
einthoven_ii_filt = ecg_class.einthoven_II_filt
126
127 #define output array and intermediate variable
filterecg = np.zeros(len(ecg)+1)
filtereinthoven = np.zeros(len(einthoven_ii)+1)
130 intermediate = 0
167 pyplot.figure(11)
168 #print(len(einthoven_ii))
time4 = np.linspace(0,len(einthoven_ii)/fs,len(einthoven_ii))
170 pyplot.plot(time4,einthoven_ii)
pyplot.title('einthoven_ii (raw)')
pyplot.xlabel('Time(s)')
173 pyplot.ylabel('Amplitude')
#pyplot.savefig('ecg_fig11.eps', format='eps')
               Listing 8: Load .dat Files and Time Domain Plot
```

#for diagnosis plot

88

89 ecg = loadtxt("ECG.dat")

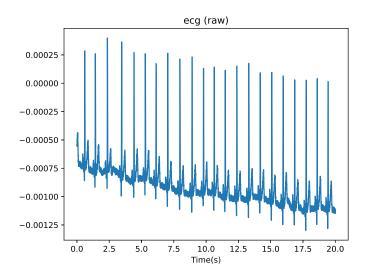


Figure 8: Raw ECG from ECG.dat

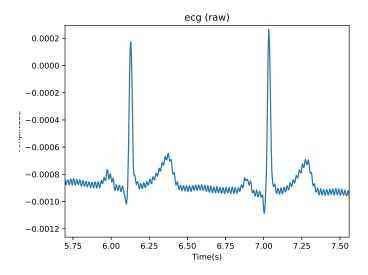


Figure 9: Partly Raw ECG from ECG.dat

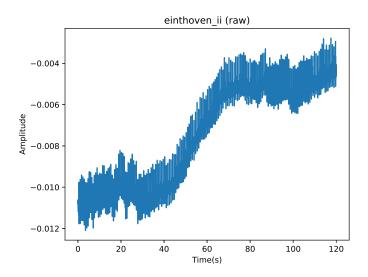


Figure 10: Raw ECG from Einthoven_ii Walking

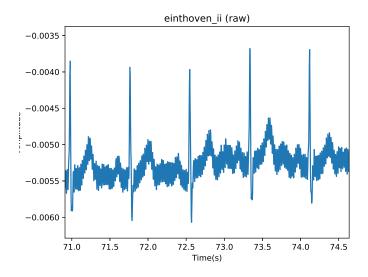


Figure 11: Partly Raw ECG from Einthoven_ii Walking

We perform both 50 Hz notch filter and DC filter to both data sets and plot the filtered ECG.

```
132 #filter ecg for both data sets
133 count = 0
```

```
134 for line in file1:
135
       count += 1
       ecg1 = line.strip()
136
       #print(ecg1)
137
       intermediate = Filter50.dofilter(ecg1)
138
       filterecg[count] = FilterDC.dofilter(intermediate)
139
140
141 for i in range(len(einthoven_ii)):
       intermediate = Filter50.dofilter(einthoven_ii[i])
142
       filtereinthoven[i] = FilterDC.dofilter(intermediate)
143
144
#print(count)
146
147 #plot the filtered data
148 pyplot.figure(9)
time2 = np.linspace(0,len(filterecg)/fs,len(filterecg))
pyplot.plot(time2,filterecg)
#pyplot.ylim(-0.002,0.002)
pyplot.title('ecg (filtered)')
pyplot.xlabel('Time(s)')
pyplot.ylabel('Amplitude')
#pyplot.savefig('ecg_fig9.eps', format='eps')
156
pyplot.figure(10)
158 time3 = np.linspace(0,len(filtereinthoven)/fs,len(filtereinthoven))
pyplot.plot(time3,filtereinthoven)
160 pyplot.ylim(-0.002,0.002)
pyplot.title('einthoven (filtered)')
pyplot.xlabel('Time(s)')
pyplot.ylabel('Amplitude')
#pyplot.savefig('ecg_fig10.eps', format='eps')
```

Listing 9: Filter operation and Filtered Time Domain Plot

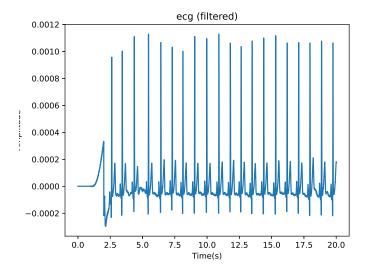


Figure 12: Filtered ECG from ECG.dat

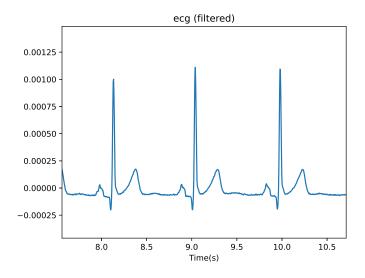


Figure 13: Partly ECG from ECG.dat

From figure 13, the ECG from the filter does still look intact.

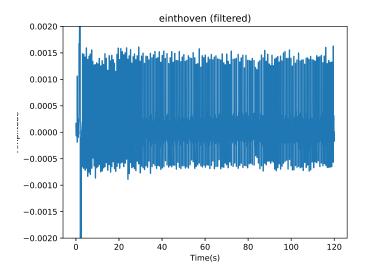


Figure 14: Filtered ECG from Einthoven_ii Walking

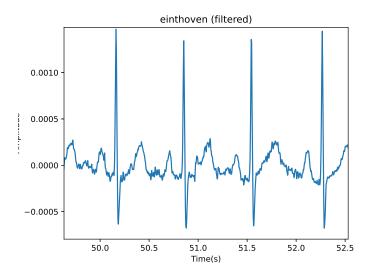


Figure 15: Partly Filtered ECG from Einthoven_ii Walking

We can see that the filtered plots are a lot cleaner and no DC line visible. The first part of both filtered ECGs are invalid because the filter is being filled up as mentioned earlier. There are about 2 heart beat loss.

We saved the processed ECG data into another .dat file to be used for heart

rate detection.

```
#save filtered data
np.savetxt('shortecg.dat',filterecg)
np.savetxt('shorteint.dat',filtereinthoven)
```

Listing 10: Save .dat Files

1.3 Discussion

We can use ring buffer to reduce computation steps required from shifting operation.

```
, , ,
2 import numpy as np
3 # Inefficient way
4 class FIR_filter:
      def __init__(self,coefficients):
          self.coeff = coefficients
          self.offset = 0
          self.buffer = np.empty(len(coefficients))
      def dofilter(self,u):
10
11
          result = 0
          for i in range(len(self.buffer)-1,0,1): #range(start,end,
12
      step)
              self.buffer[i+1] = self.buffer[i]
          self.buffer[0] = u
14
          for i in range(len(self.buffer)-1):
15
              result = result + self.coeff[i] * self.buffer[i]
16
          return result
17
18 ,,,
```

Listing 11: Not Using Ring Buffer Version

The fundamental frequency of the ECG starts around 1 Hz, so the cutoff frequency should be below 1 Hz to avoid eliminating the ECG signal itself.

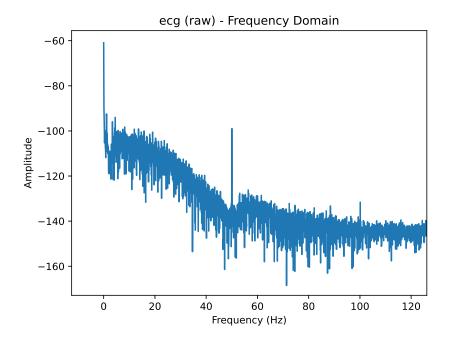


Figure 16: Raw ECG in Frequency Domain from ECG.dat

From figure 16, we could observe peak at 0 Hz (DC) and a peak at 50 Hz noise. The other spectrum amplitude is high near lower frequencies which implies that the ECG signal composes of lower frequencies. To conclude, from this frequency domain plot of the spectrum, we could decide on which cutoff frequencies should be used in our filter design.

2 HeartRate Detection

2.1 Introduction

Detecting heart-rate peaks from the ECG data requires a DC free signal, so we used the data processed from the previous ecg_filter.py. The template is created by trimming one of a PQRST from the corresponding ECG. Then inverse of the template is used as the coefficient of the FIR Filter. An anti-noise heartbeat algorithm is implemented to the code to prevent noise detected as an extra irregular heartbeat. Time difference from one peak to another is processed to get the beats per minute.

Einthoven ii walking ECG recording, which provides greater noise as a benchmark test of the noise filtering, is loaded to test the heart-rate detection program.

2.2 Method and Results

```
1 import numpy as np
2 from matplotlib import pyplot
3 from numpy import loadtxt
4 from fir_filter import FIR_filter
6 \text{ Case} = 0
7 #Case = int(input("Case 0 For shortecg.dat. Case 1 For Einthoven_ii
       Walking. Please enter case number: "))
8 for Case in range (2):
       if Case == 0:
           cleanecg = loadtxt("shortecg.dat")
10
       if Case == 1:
11
           cleanecg = loadtxt("shorteint.dat")
12
13
      fs=250
                   #sampling frequency of the data
14
15
16
      pyplot.figure(8*Case+1)
      time = np.linspace(0, len(cleanecg)/fs, len(cleanecg))
17
      pyplot.plot(time,cleanecg)
18
      pyplot.title('ecg (filtered)')
19
      pyplot.xlabel('Time(s)')
20
21
      pyplot.ylabel('Amplitude')
       # if Case == 0:
22
23
            pyplot.savefig('hr_fig1.eps', format='eps')
      # if Case == 1:
24
            pyplot.savefig('hr_fig9.eps', format='eps')
25
26
      #ecg templates for each data set
27
       if Case == 0:
28
          template=cleanecg[775:975]
29
30
       if Case == 1:
           template=cleanecg[7050:7225]
31
32
      #plot template
33
      pyplot.figure(8*Case+2)
34
       time2 = np.linspace(0,len(template)/fs,len(template))
35
       pyplot.plot(time2,template)
36
      pyplot.title('1 ecg')
37
38
      pyplot.xlabel('Time(s)')
      pyplot.ylabel('Amplitude')
39
       # if Case == 0:
40
             pyplot.savefig('hr_fig2.eps', format='eps')
41
       # if Case == 1:
42
            pyplot.savefig('hr_fig10.eps', format='eps')
43
44
45
       #inverse the template
      fir_coeff = template[::-1]
46
47
      pyplot.figure(8*Case+3)
      pyplot.plot(time2,fir_coeff)
48
      pyplot.title('reversed 1 ecg')
49
      pyplot.xlabel('Time(s)')
50
      pyplot.ylabel('Amplitude')
51
       # if Case == 0:
      #
            pyplot.savefig('hr_fig3.eps', format='eps')
53
      # if Case == 1:
54
```

Listing 12: Obtaining Coefficient for FIR filter

Two cases are implemented to switch between the shortecg.dat and the Einthoven II walking ECG. The templates were eye-observed from the graphs, and then trimmed for the length of one PQRST Complex. Then the template is inversed corresponding the x-axis.

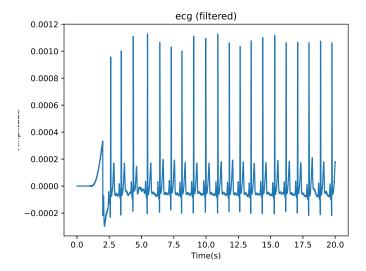


Figure 17: Filtered ECG from ECG.dat

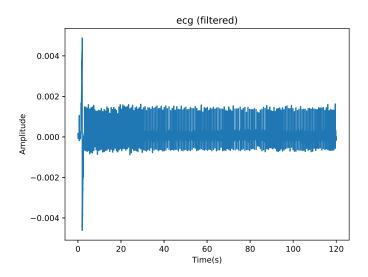


Figure 18: Filtered ECG from Einthoven_ii Walking

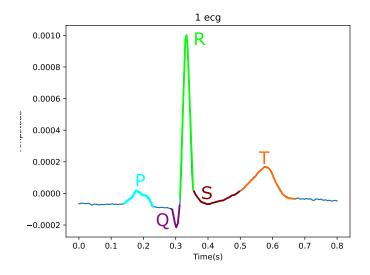


Figure 19: 1 ECG from ECG.dat

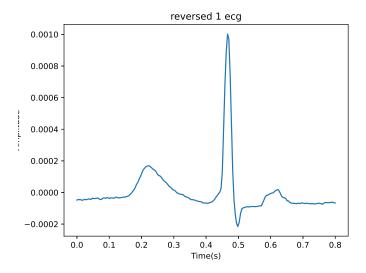


Figure 20: Reversed 1 ECG from ECG.dat

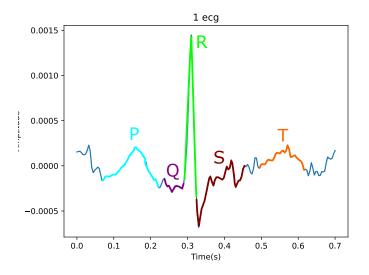


Figure 21: 1 ECG from Einthoven_ii Walking

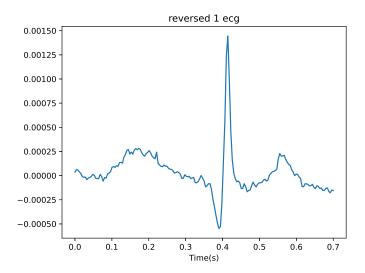


Figure 22: Reversed 1 ECG from Einthoven_ii Walking

```
#matched filtered data
57
      matchfilt = FIR_filter(fir_coeff)
58
59
      matchresult = np.zeros(len(cleanecg))
60
      for i in range(len(cleanecg)):
61
62
           matchresult[i] = matchfilt.dofilter(cleanecg[i])
      pyplot.figure(8*Case+4)
64
      pyplot.plot(time, matchresult)
65
      pyplot.title('Matched Filtered ecg')
66
      pyplot.xlabel('Time(s)')
67
      pyplot.ylabel('Amplitude')
68
        if Case == 0:
69
             pyplot.savefig('hr_fig4.eps', format='eps')
70
      # if Case == 1:
71
             pyplot.savefig('hr_fig12.eps', format='eps')
72
      print(len(matchresult))
```

Listing 13: Matched Filter Implementation

FIR Filter is used to perform matched filter. The coefficients are the inverted template, which is the **fir-coeff**.

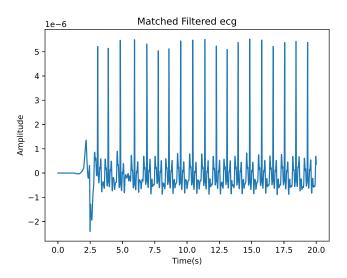


Figure 23: Match Filter Result from ECG.dat

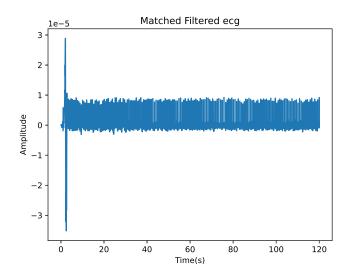


Figure 24: Match Filter Result from Einthoven_ii Walking

```
#squared matched filtered data
matchresult = matchresult*matchresult
pyplot.figure(8*Case+5)
pyplot.plot(time,matchresult) #
pyplot.title('Squared Matched Filtered ecg')
```

```
pyplot.xlabel('Time(s)')
pyplot.ylabel('Amplitude')

# if Case == 0:
# pyplot.savefig('hr_fig5.eps', format='eps')
# if Case == 1:
# pyplot.savefig('hr_fig13.eps', format='eps')
```

Listing 14: Squaring the Results

By squaring the matched results post-filter, the outcome of the data produces higher peak with lower noise.

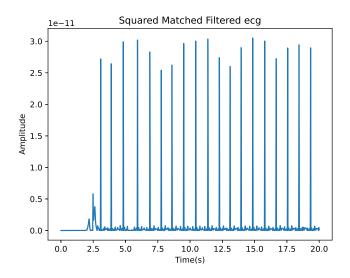


Figure 25: Squared Match Filter Result from ECG.dat

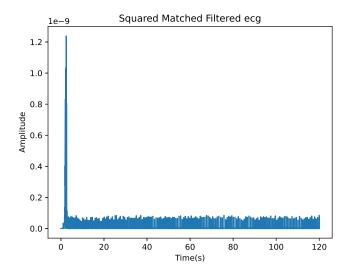


Figure 26: Squared Match Filter Result from Einthoven_ii Walking

```
#using threshold to extract the peaks
87
       hr = np.zeros(len(matchresult))
88
       threshold = 0.00000000002
89
       for i in range(len(matchresult)):
90
           if matchresult[i]>threshold:
91
               hr[i]=1
92
93
       pyplot.figure(8*Case+6)
94
       pyplot.plot(hr)
95
       pyplot.title('Heart Beat Detection Sequence')
96
       pyplot.xlabel('Sample number')
97
       pyplot.ylabel('Amplitude')
98
       #pyplot.xlim(3,120)
                                         #to delete the first part where
99
        the buffer is being filled/diagnosis purpose
       # if Case == 0:
              pyplot.savefig('hr_fig6.eps', format='eps')
101
       # if Case == 1:
             pyplot.savefig('hr_fig14.eps', format='eps')
103
```

Listing 15: Peak Threshold

The threshold used to detect the peaks of the data is around

```
2.0*10^{-}11
```

The value was observed from time domain plot of the squared matched result.

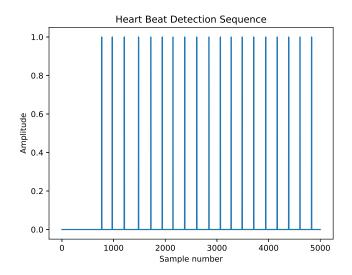


Figure 27: Heart Beat Extraction using Threshold from ECG.dat

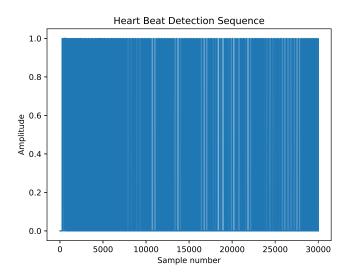


Figure 28: Heart Beat Extraction using Threshold from Einthoven_ii Walking

```
#initiate counters

peakCounter = 0  #count number of peaks > for array size

detectIndex = 0  #detection index

deltatIndex = 0  #deltat index
```

```
index = np.zeros(len(hr))
110
       threshT = int(1/(3.66/fs))
                                       #3.66beat/s is the maximum heart
111
       rate(220bpm)
112
       for i in range(len(hr)):
113
           if hr[i] == 1:
114
                peakCounter+=1
                for n in range(int(threshT)):
                                                   #fix the impossible
       detected peak to 0
                    if i+n+1 <= 30000:</pre>
117
                                                  #If the time is less
       than 30000
                        hr[i+n+1] = 0
118
119
       pyplot.figure(8*Case+7)
120
       pyplot.plot(hr)
121
       pyplot.title('Heart Beat Detection Sequence Fixed')
122
       pyplot.xlabel('Sample number')
       pyplot.ylabel('Amplitude')
124
125
       #pyplot.xlim(3,120)
                                     #to delete the first part where the
        buffer is being filled/diagnosis purpose
       # if Case == 0:
             pyplot.savefig('hr_fig7.eps', format='eps')
       # if Case == 1:
128
             pyplot.savefig('hr_fig15.eps', format='eps')
129
```

Listing 16: Time Threshold

A time threshold **threshT** is used to delete unwanted/false 1s sequence between two peaks. A constant value of 3.66 beat/s is the highest heart-rate that would occur. The threshold is interpolated into the array index length. For any second detected 1s within that time threshold will be set to zero.

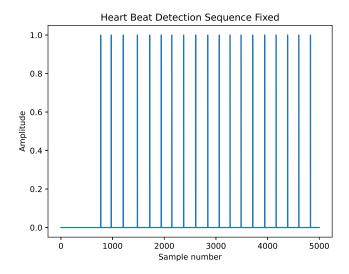


Figure 29: Heart Beat Extraction False 1s Deleted from ECG.dat

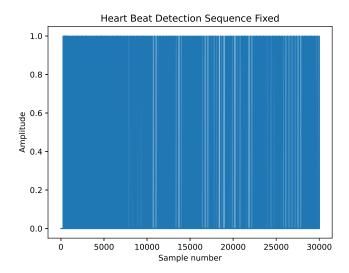


Figure 30: Heart Beat Extraction False 1s Deleted from Einthoven_ii Walking

From figure 31, we can see the 1s from the sequence is more than 1 due to the use of amplitude threshold. It's then proven to be fixed in figure 32 with the correction algorithm. Any other false peak in between time threshold would also get deleted.

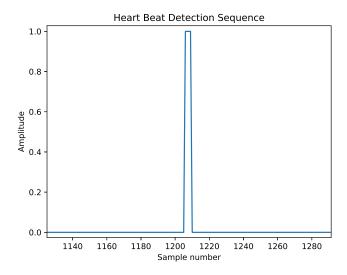


Figure 31: Partly Heart Beat Extraction using Threshold from ECG.dat

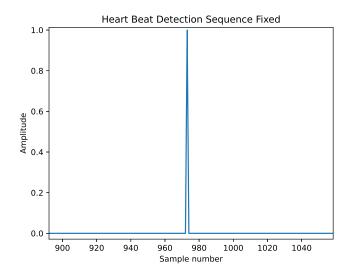


Figure 32: Partly Heart Beat Extraction False 1s Deleted from ECG.dat

```
131
       beatone = np.zeros(peakCounter)
       deltat = np.zeros(peakCounter)
       rate = np.zeros(peakCounter)
133
       print("Momentary Heart Rate(BPM)")
136
       for i in range(len(hr)):
           if hr[i] != 0:
                                     # When element is not zero, input
       element to new array
               beatone[detectIndex] = i
138
               detectIndex += 1
139
140
               if detectIndex >= 0:
                                               # To neglect the first
       detection
                    deltat[deltatIndex] = (beatone[deltatIndex] -
       beatone[deltatIndex-1])/fs
                    # print('ONE', beatone[deltatIndex])
                                                                #for
142
       diagnosis purpose
                    # print('TWO', beatone[deltatIndex -1])
143
                    # print('TIME',deltat[deltatIndex])
144
                    rate[deltatIndex] = (1/deltat[deltatIndex])*60
145
                    print(rate[deltatIndex])
146
                    deltatIndex += 1
147
148
       pyplot.figure(8*Case+8)
149
       pyplot.plot(beatone/fs,rate)
151
       pyplot.title('Heart Rate Plot')
       pyplot.xlabel('Time(s)')
       pyplot.ylabel('Beats/Minute')
153
154
       #pyplot.xlim(4,max(beatone)/fs+1)
                                                  #to delete the first
       part where the buffer is being filled/diagnosis purpose
       # if Case == 0:
       #
             pyplot.savefig('hr_fig8.eps', format='eps')
156
       # if Case == 1:
```

Listing 17: Momentary Heart Rate Calculation

To calculate the Momentary Heart Rate (BPM), the time difference **deltat** is extracted from the sequence and then calculated into BPM.

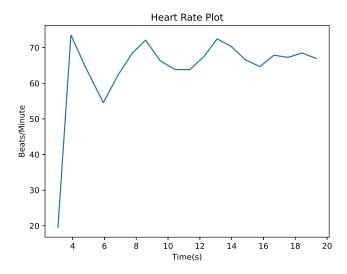


Figure 33: Momentary Heart Rate Plot from ECG.dat

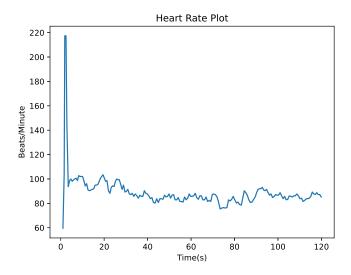


Figure 34: Momentary Heart Rate Plot from Einthoven_ii Walking

To comply with real-time processing, we have also implemented a real time heart rate detection python class using all above principle. Small changes are made to **deltat** and is replaced by **self.counter** which resets itself everytime a new peak is detected. The **threshold** also was lowered to make it be able to detect heart beat from eintoven ii data. Note that the data input into the filter instantiated from the class should be filtered by the 50 Hz notch and DC line elimination filter first. And the file submitted would only run this part to display only the momentary rate graph. It also represents how it will be used in real application. The result looks similar to figure 33 and figure 34, but only plotting at when the new heart beat has arrived and the momentary heart rate can be calculated.

```
161 class HR_filter:
       def __init__(self,):
162
           ecg = loadtxt("shortecg.dat")
                                                      #file which the
       template is extracted from
           template=ecg[775:975]
                                                      #1ecg of the
164
       corresponding file
           fir_coeff = template[::-1]
                                                       #reverse template
           self.matchfilt = FIR_filter(fir_coeff)
166
           self.hr = 0
167
           self.hrBuffer = 0
                                                      #keep previous hr
       value for peak starts checking
           self.counter = 0
                                                      #counts time
       difference before next peak arrive
       def realtimeHR(self,data,fs):
           matchresult = self.matchfilt.dofilter(data)
           matchresult = matchresult*matchresult
173
           threshold = 0.00000000001
                                                      #observed by eye
174
       from graph
176
           #use threshold to extract peak area
           if matchresult>threshold:
177
                self.hr=1
178
            else:
179
                self.hr=0
180
181
           threshT = int(1/(3.66/fs))
                                                       #3.66beat/s is the
182
        maximum heart rate(220bpm)
                                                      #default argument
           rate=0
183
184
           #checks if the peak starts
185
           if self.hrBuffer == 0 and self.hr == 1:
186
                #peak=1
                           #for diagnosis purpose : peak starts
187
188
                if self.counter>threshT:
                    rate = (fs/self.counter)*60
189
190
                    self.counter=0
                                                           #reset counter
                return rate
191
192
                #peak=0
                              #for diagnosis purpose : no peak starting
                self.counter+=1
194
                return None
           #return matchresult
196
           self.hrBuffer = self.hr
                                                      #save value for
```

```
future comparison
199
200 #Example Use
201 data = loadtxt("shortecg.dat")
202 data2 = loadtxt("shorteint.dat")
203 fs=250
204 mhr = np.zeros(len(data))
205 mhr2 = np.zeros(len(data2))
                                                   #instantiate the
206 hrfilt = HR_filter()
      HR_filter
207 for i in range(len(data)):
    mhr[i] = hrfilt.realtimeHR(data[i],fs)
208
209 for i in range(len(data2)):
      mhr2[i] = hrfilt.realtimeHR(data2[i],fs)
211
212 pyplot.figure(17)
pyplot.plot(np.linspace(0,len(data)/fs,len(data)),mhr)
214 pyplot.title('Momentary Heart Rate Plot from ECG.dat')
pyplot.xlabel('Time(s)')
216 pyplot.ylabel('Beats/Minute')
#pyplot.savefig('hr_fig17.eps', format='eps')
218
219 pyplot.figure(18)
pyplot.plot(np.linspace(0,len(data2)/fs,len(data2)),mhr2)
pyplot.title('Momentary Heart Rate Plot from einthoven II')
222 pyplot.xlabel('Time(s)')
pyplot.ylabel('Beats/Minute')
#pyplot.savefig('hr_fig18.eps', format='eps')
```

Listing 18: Momentary Heart Rate Calculation

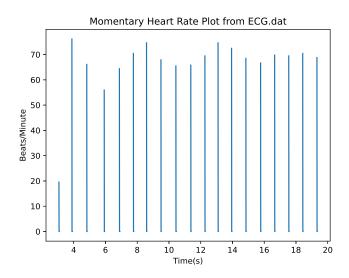


Figure 35: Momentary Heart Rate Plot from shortecg.dat using filter class implemented

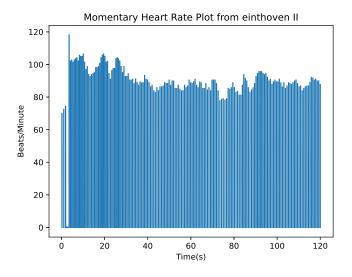


Figure 36: Momentary Heart Rate Plot from shorteint. dat using filter class implemented $\,$

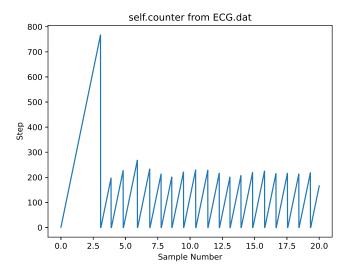


Figure 37: self.counter Uses of Detecting Heart Beat from shortecg.dat

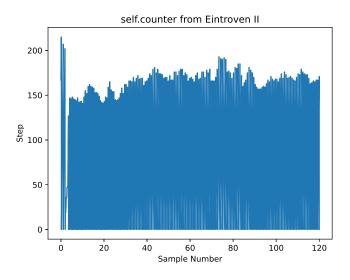


Figure 38: self.counter Uses of Detecting Heart Beat from shorteint.dat

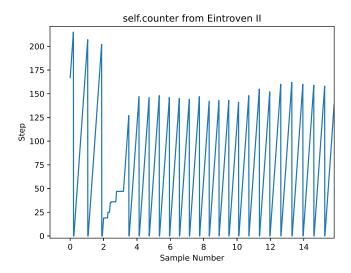


Figure 39: Partly self.counter Uses of Detecting Heart Beat from shorteint.dat

2.3 Discussion

Figure 20 shows the use of time-inversed template for the matched filter, as it indicates PQRST points on the template. The template is time-reversed to fulfil the requirements to perform convolution with the input signal. The template taken from one of the PQRST complex is then used as the coefficient to perform a matched filter to the data. Results of the match filter on figure 23 shows an increase of the ratio of the peaks to the noise. After squaring the data, a threshold is applied to the data to capture the peaks, which can be seen on figure 27. The detected sequence are in form of an array which consists of ones and zeros. The detected heart-rate plot on figure 32 shows the trends of the Beats Per Minute under 20 seconds of the sampled data.

The Einthoven II walking data is presumed to have greater noise occurring throughout the 50Hz, which may disrupt the R-peak detection. On figure 21 we indicate the PQRST complex on the template sampled from the Einthoven II which looks obviously more noisy than that of the shortecg.dat one. Figure 24 is the reversed template. Under the same process alike the shortecg.dat data, we use square matched filter and thresholds application to refine the peaks of the beats. After the calculation of the Beats/Minute, the momentary heart rate plot is shown on figure 28 within 120 seconds. Note that the array taken to complete the full buffer invalidate the value on the early times when the buffer is being filled up. Again, a trade-off is introduced between frequency resolution and the length of data being invalidated by the buffer.

We can actually use a same template for any data as demonstrated by the python class implemented. It doesn't matter which data the template is ex-

tracted from, but the template must represent an ECG signal(with all the ECG artefacts/PQRST).

As the outcome, the python class instantiated filter successfully detected the heartrate of the Einthoven II walking with lower **threshold**.

In addition, we tried to plot the raw vs. filtered data of a more noisy database. From figure 40, the raw data in orange obviously demonstrate a DC line shift, while the filtered one line shift is eliminated by the filters applied in ecg_filter.py. When it is used in hr_detect.py, the line shift will not affect the matched filter result.

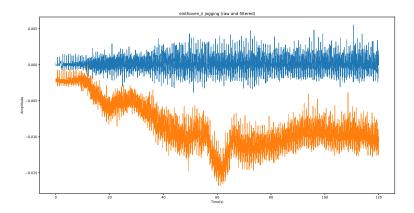


Figure 40: Raw vs. Filtered data from Einthoven_ii Jogging

3 Appendix

3.1 fir_filter.py

```
import numpy as np
  # Inefficient way
  class FIR_filter:
      def __init__(self,coefficients):
          self.coeff = coefficients
          self.offset = 0
          self.buffer = np.empty(len(coefficients))
      def dofilter(self,u):
10
          result = 0
          for i in range(len(self.buffer)-1,0,1): #range(start,end,
12
               self.buffer[i+1] = self.buffer[i]
13
          self.buffer[0] = u
14
          for i in range(len(self.buffer)-1):
15
               result = result + self.coeff[i] * self.buffer[i]
```

```
return result
17
18
19 ,,,
20 import numpy as np
21 class FIR_filter:
      def __init__(self,coefficients):
22
           self.coeff = coefficients
23
          self.offset = 0
24
          self.buffer = np.zeros(len(coefficients))
25
26
      def dofilter(self,u):
27
28
          result = 0
          self.buffer[self.offset] = u
29
30
          #print("offset index:", self.offset)
31
          for i in range(self.offset+1):
32
               result = result + self.buffer[i]*self.coeff[self.offset
33
      -i]
34
               #print("buffer index:",i)
               #print("coeff index:",self.offset-i)
35
          #print("Second For Section")
37
          for i in range(self.offset+1,len(self.buffer),1):
38
39
               result = result + self.buffer[i]*self.coeff[len(self.
      buffer) -1+self.offset+1-i]
40
               #print("buffer index:",i)
               #print("coeff index:",len(self.buffer)-1+self.offset+1-
41
      i)
42
           self.offset+=1
43
           if self.offset>=len(self.buffer):
44
               self.offset=0
45
46
          return result
47
48
49
      def dofilterPrint(self,u):
                                      #index printing version for
      diagnosis purpose
50
          result = 0
          self.buffer[self.offset] = u
51
52
          print("offset index:",self.offset)
53
54
          for i in range(self.offset+1):
               result = result + self.buffer[i]*self.coeff[self.offset
55
      -i]
               print("buffer index:",i)
56
               print("coeff index:",self.offset-i)
57
58
59
           print("Second For Section")
          for i in range(self.offset+1,len(self.buffer),1):
60
               result = result + self.buffer[i]*self.coeff[len(self.
      buffer) -1+self.offset+1-i]
               print("buffer index:",i)
62
               print("coeff index:",len(self.buffer)-1+self.offset+1-i
63
      )
           self.offset+=1
65
          if self.offset>=len(self.buffer):
```

```
self.offset=0
67
          return result
69
70
71 def unittest():
          h = np.array([1/2,1/2,0,0,0])
72
          print("Coefficient:",h)
73
          f = FIR_filter(h)
74
          y= f.dofilterPrint(0)
                                       #use the index printing version
          print("Input 0, Output",y)
76
          y= f.dofilterPrint(1)
                                       #use the index printing version
77
          print("Input 1, Output",y)
78
          for i in range (20):
79
                                       #use the index printing version
              y= f.dofilterPrint(0)
              print("Input 0, Output",y)
81
82
83 if __name__ == "__main__":
84 unittest()
```

Listing 19: fir_filter.py

3.2 ecg_filter.py

```
1 from ecg_gudb_database import GUDb
2 import numpy as np
3 from fir_filter import FIR_filter
4 from numpy import loadtxt
5 from matplotlib import pyplot
7 \text{ fs} = 250
               #Hz
8 M = 500
              #loses 2 heart beat to warm up the filter (2seconds)/
      affect frequency resolution
10 # 50 Hz Notch Filter
11 k1 = int(49.5/fs * M)
12 k2 = int(50.5/fs * M)
14 Window50 = np.ones(M)
15 Coeff50 = np.ones(M)
17 \text{ Window50[k1:k2+1]} = 0
18 Window50 [M-k2:M-k1+1] = 0
20 pyplot.figure(1)
pyplot.plot(Window50)
pyplot.title('50 Hz Notch Filter - Ideal')
23 pyplot.xlabel('M (sample number)')
pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig1.eps', format='eps')
W50 = np.fft.ifft(Window50)
28 W50 = np.real(W50)
30 pyplot.figure(2)
31 pyplot.plot(W50)
32 pyplot.title('50 Hz Notch Filter - IFFT')
```

```
33 pyplot.xlabel('Coefficient Index')
34 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig2.eps', format='eps')
37 Coeff50[0:int(M/2)] = W50[int(M/2):M]
38 Coeff50[int(M/2):M] = W50[0:int(M/2)]
40 pyplot.figure(3)
41 pyplot.plot(Coeff50)
42 pyplot.title('50 Hz Notch Filter - IFFT(fixed)')
43 pyplot.xlabel('Coefficient Index')
44 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig3.eps', format='eps')
47 Filter50 = FIR_filter(Coeff50)
49
50 #DC filter
k3 = int(0.5/fs * M)
52 WindowDC = np.ones(M)
53 CoeffDC = np.ones(M)
55 WindowDC[0:k3+1] = 0
56 pyplot.figure(4)
57 pyplot.plot(WindowDC)
58 pyplot.title('DC Filter - Ideal')
59 pyplot.xlabel('M (sample number)')
60 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig4.eps', format='eps')
62
63 WDC = np.fft.ifft(WindowDC)
64 WDC = np.real(WDC)
66 pyplot.figure(5)
67 pyplot.plot(WDC)
68 pyplot.title('DC Filter - IFFT')
69 pyplot.xlabel('Coefficient Index')
70 pyplot.ylabel('Amplitude')
71 # pyplot.savefig('ecg_fig5.eps', format='eps')
73 CoeffDC[0:int(M/2)] = WDC[int(M/2):M]
74 CoeffDC[int(M/2):M] = WDC[0:int(M/2)]
76 pyplot.figure(6)
77 pyplot.plot(CoeffDC)
78 pyplot.title('DC Filter - IFFT(fixed)')
79 pyplot.xlabel('Coefficient Index')
80 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig6.eps', format='eps')
83 FilterDC = FIR_filter(CoeffDC)
84
86 # load first ECG file
87 file1 = open('ECG.dat', 'r')
                                    #line by line to use as real-time
      filter
```

```
89 ecg = loadtxt("ECG.dat") #for diagnosis plot
91 pyplot.figure(7)
92 #print(len(ecg))
193 time = np.linspace(0,len(ecg)/fs,len(ecg))
94 pyplot.plot(time,ecg)
95 pyplot.title('ecg (raw)')
96 pyplot.xlabel('Time(s)')
97 pyplot.ylabel('Amplitude')
98 # pyplot.savefig('ecg_fig7.eps', format='eps')
100
101 # Investigate frequency domain
102 fx=np.fft.fft(ecg)
103 fxx = fx/len(ecg)
                                 # Fourier Transform Normalised
104 dbs = 20*np.log10(abs(fxx)) # DB Conversion
105 pyplot.figure(8)
freq = np.linspace(0,fs,len(ecg))
107 pyplot.plot(freq,dbs)
108 pyplot.title('ecg (raw) - Frequency Domain')
109 pyplot.xlabel('Frequency (Hz)')
pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig8.eps', format='eps')
112
113 #load second ECG data
^{114} '''Initialise experiments from the files of einthoven'''
subject_number = 3
116 experiment = 'walking'
ecg_class = GUDb(subject_number, experiment)
118
''', Initialise experiments from the files of einthoven''',
chest_strap_V2_V1 = ecg_class.cs_V2_V1
121 einthoven_ii = ecg_class.einthoven_II
'', Filtered Data With Einthoven',
124 ecg_class.filter_data()
einthoven_ii_filt = ecg_class.einthoven_II_filt
127 #define output array and intermediate variable
128 filterecg = np.zeros(len(ecg)+1)
filtereinthoven = np.zeros(len(einthoven_ii)+1)
130 intermediate = 0
131
_{\rm 132} #filter ecg for both data sets
133 count = 0
134 for line in file1:
      count += 1
135
136
       ecg1 = line.strip()
       #print(ecg1)
137
       intermediate = Filter50.dofilter(ecg1)
138
       filterecg[count] = FilterDC.dofilter(intermediate)
139
140
141 for i in range(len(einthoven_ii)):
       intermediate = Filter50.dofilter(einthoven_ii[i])
142
       filtereinthoven[i] = FilterDC.dofilter(intermediate)
143
144
145 #print(count)
```

```
146
#plot the filtered data
148 pyplot.figure(9)
time2 = np.linspace(0,len(filterecg)/fs,len(filterecg))
pyplot.plot(time2,filterecg)
#pyplot.ylim(-0.002,0.002)
152 pyplot.title('ecg (filtered)')
pyplot.xlabel('Time(s)')
pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig9.eps', format='eps')
pyplot.figure(10)
time3 = np.linspace(0,len(filtereinthoven)/fs,len(filtereinthoven))
pyplot.plot(time3,filtereinthoven)
160 pyplot.ylim(-0.002,0.002)
pyplot.title('einthoven (filtered)')
162 pyplot.xlabel('Time(s)')
pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig10.eps', format='eps')
165
167 pyplot.figure(11)
168 #print(len(einthoven_ii))
time4 = np.linspace(0,len(einthoven_ii))fs,len(einthoven_ii))
pyplot.plot(time4,einthoven_ii)
pyplot.title('einthoven_ii (raw)')
172 pyplot.xlabel('Time(s)')
173 pyplot.ylabel('Amplitude')
# pyplot.savefig('ecg_fig11.eps', format='eps')
175
177 #save filtered data
np.savetxt('shortecg.dat',filterecg)
np.savetxt('shorteint.dat',filtereinthoven)
```

Listing 20: ecg_filter.py

3.3 hr_detect.py

```
1 import numpy as np
from matplotlib import pyplot
3 from numpy import loadtxt
4 from fir_filter import FIR_filter
5 ,,,
6 \text{ Case} = 0
7 #Case = int(input("Case 0 For shortecg.dat. Case 1 For Einthoven_ii
      Walking. Please enter case number: "))
8 for Case in range (2):
      if Case == 0:
          cleanecg = loadtxt("shortecg.dat")
10
      if Case == 1:
11
          cleanecg = loadtxt("shorteint.dat")
12
13
14
      fs = 250
                  #sampling frequency of the data
15
pyplot.figure(8*Case+1)
```

```
time = np.linspace(0,len(cleanecg)/fs,len(cleanecg))
17
      pyplot.plot(time,cleanecg)
18
      pyplot.title('ecg (filtered)')
19
      pyplot.xlabel('Time(s)')
20
      pyplot.ylabel('Amplitude')
21
      # if Case == 0:
22
23
            pyplot.savefig('hr_fig1.eps', format='eps')
      # if Case == 1:
24
           pyplot.savefig('hr_fig9.eps', format='eps')
25
26
27
      #ecg templates for each data set
28
      if Case == 0:
          template=cleanecg[775:975]
29
      if Case == 1:
          template=cleanecg[7050:7225]
31
32
33
      #plot template
      pyplot.figure(8*Case+2)
34
      time2 = np.linspace(0,len(template)/fs,len(template))
      pyplot.plot(time2,template)
36
      pyplot.title('1 ecg')
37
      pyplot.xlabel('Time(s)')
38
      pyplot.ylabel('Amplitude')
39
40
      # if Case == 0:
            pyplot.savefig('hr_fig2.eps', format='eps')
41
      # if Case == 1:
42
            pyplot.savefig('hr_fig10.eps', format='eps')
43
44
45
      #inverse the template
      fir_coeff = template[::-1]
46
      pyplot.figure(8*Case+3)
47
      pyplot.plot(time2,fir_coeff)
48
      pyplot.title('reversed 1 ecg')
49
      pyplot.xlabel('Time(s)')
50
      pyplot.ylabel('Amplitude')
51
52
      # if Case == 0:
            pyplot.savefig('hr_fig3.eps', format='eps')
53
54
      # if Case == 1:
           pyplot.savefig('hr_fig11.eps', format='eps')
55
56
57
      #matched filtered data
      matchfilt = FIR_filter(fir_coeff)
58
      matchresult = np.zeros(len(cleanecg))
60
      for i in range(len(cleanecg)):
61
62
          matchresult[i] = matchfilt.dofilter(cleanecg[i])
63
      pyplot.figure(8*Case+4)
64
      pyplot.plot(time, matchresult)
65
      pyplot.title('Matched Filtered ecg')
66
      pyplot.xlabel('Time(s)')
67
      pyplot.ylabel('Amplitude')
68
69
      # if Case == 0:
            pyplot.savefig('hr_fig4.eps', format='eps')
70
71
      # if Case == 1:
            pyplot.savefig('hr_fig12.eps', format='eps')
72
print(len(matchresult))
```

```
74
75
       #squared matched filtered data
       matchresult = matchresult*matchresult
76
       pyplot.figure(8*Case+5)
77
       pyplot.plot(time, matchresult)
78
       pyplot.title('Squared Matched Filtered ecg')
79
       pyplot.xlabel('Time(s)')
80
       pyplot.ylabel('Amplitude')
81
       # if Case == 0:
82
             pyplot.savefig('hr_fig5.eps', format='eps')
83
       # if Case == 1:
84
             pyplot.savefig('hr_fig13.eps', format='eps')
85
86
       #using threshold to extract the peaks
87
       hr = np.zeros(len(matchresult))
88
       threshold = 0.00000000002
89
90
       for i in range(len(matchresult)):
           if matchresult[i]>threshold:
91
92
               hr[i]=1
93
       pyplot.figure(8*Case+6)
94
       pyplot.plot(hr)
95
       pyplot.title('Heart Beat Detection Sequence')
96
       pyplot.xlabel('Sample number')
97
       pyplot.ylabel('Amplitude')
98
                                        #to delete the first part where
99
       #pyplot.xlim(3,120)
        the buffer is being filled/diagnosis purpose
       # if Case == 0:
100
             pyplot.savefig('hr_fig6.eps', format='eps')
       # if Case == 1:
102
103
              pyplot.savefig('hr_fig14.eps', format='eps')
104
       #initiate counters
       peakCounter = 0  #count number of peaks > for array size
106
       detectIndex = 0
                         #detection index
107
                        #deltat index
       deltatIndex = 0
108
109
       index = np.zeros(len(hr))
       threshT = int(1/(3.66/fs))
                                    #3.66beat/s is the maximum heart
111
       rate(220bpm)
112
113
       for i in range(len(hr)):
           if hr[i] == 1:
114
               peakCounter+=1
               for n in range(int(threshT)):
                                                 #fix the impossible
116
       {\tt detected\ peak\ to\ 0}
                   if i+n+1 <= 30000:
                                                 #If the time is less
117
       than 30000
                       hr[i+n+1] = 0
118
119
       pyplot.figure(8*Case+7)
120
       pyplot.plot(hr)
121
       pyplot.title('Heart Beat Detection Sequence Fixed')
122
       pyplot.xlabel('Sample number')
123
       pyplot.ylabel('Amplitude')
124
       #pyplot.xlim(3,120)
                                    #to delete the first part where the
125
      buffer is being filled/diagnosis purpose
```

```
# if Case == 0:
126
127
             pyplot.savefig('hr_fig7.eps', format='eps')
       # if Case == 1:
128
            pyplot.savefig('hr_fig15.eps', format='eps')
129
130
       beatone = np.zeros(peakCounter)
131
       deltat = np.zeros(peakCounter)
132
       rate = np.zeros(peakCounter)
       print("Momentary Heart Rate(BPM)")
135
136
       for i in range(len(hr)):
           if hr[i] != 0:
137
                                    # When element is not zero, input
       element to new array
               beatone[detectIndex] = i
138
               detectIndex += 1
139
               if detectIndex >= 0:
                                               # To neglect the first
140
       detection
                   deltat[deltatIndex] = (beatone[deltatIndex] -
141
       beatone[deltatIndex-1])/fs
                   # print('ONE', beatone[deltatIndex])
                                                               #for
142
       diagnosis purpose
                   # print('TWO', beatone[deltatIndex -1])
143
                    # print('TIME',deltat[deltatIndex])
144
145
                   rate[deltatIndex] = (1/deltat[deltatIndex])*60
                   print(rate[deltatIndex])
146
                    deltatIndex += 1
147
148
       pyplot.figure(8*Case+8)
149
       pyplot.plot(beatone/fs,rate)
150
       pyplot.title('Heart Rate Plot')
       pyplot.xlabel('Time(s)')
       pyplot.ylabel('Beats/Minute')
153
       #pyplot.xlim(4,max(beatone)/fs+1)
                                                 #to delete the first
154
       part where the buffer is being filled/diagnosis purpose
       # if Case == 0:
156
             pyplot.savefig('hr_fig8.eps', format='eps')
       # if Case == 1:
157
158
           pyplot.savefig('hr_fig16.eps', format='eps')
159
160
161 class HR_filter:
       def __init__(self,):
162
           ecg = loadtxt("shortecg.dat")
                                                     #file which the
163
       template is extracted from
           template=ecg[775:975]
                                                     #1ecg of the
164
       corresponding file
          fir_coeff = template[::-1]
                                                     #reverse template
           self.matchfilt = FIR_filter(fir_coeff)
166
           self.hr = 0
167
           self.hrBuffer = 0
                                                     #keep previous hr
168
       value for peak starts checking
           self.counter = 0
                                                     #counts time
       difference before next peak arrive
170
171
       def realtimeHR(self,data,fs):
           matchresult = self.matchfilt.dofilter(data)
172
           matchresult = matchresult*matchresult
173
```

```
threshold = 0.00000000001
                                        #observed by eye
174
       from graph
175
           #use threshold to extract peak area
176
           if matchresult>threshold:
               self.hr=1
178
179
           else:
               self.hr=0
180
181
           threshT = int(1/(3.66/fs))
                                                     #3.66beat/s is the
182
        maximum heart rate(220bpm)
           rate=0
                                                    #default argument
183
184
           #checks if the peak starts
185
           if self.hrBuffer==0 and self.hr==1:
186
               #peak=1
                          #for diagnosis purpose : peak starts
187
188
               if self.counter>threshT:
                   rate = (fs/self.counter)*60
189
190
                   self.counter=0
                                                        #reset counter
               return rate
191
           else:
               #peak=0
                            #for diagnosis purpose : no peak starting
193
               self.counter+=1
195
               return None
           #return matchresult
196
           self.hrBuffer = self.hr
                                                    #save value for
197
       future comparison
198
199
200 #Example Use
201 data = loadtxt("shortecg.dat")
202 data2 = loadtxt("shorteint.dat")
203 fs=250
204 mhr = np.zeros(len(data))
205 mhr2 = np.zeros(len(data2))
206 hrfilt = HR_filter()
                                                     #instantiate the
      HR_filter
207 for i in range(len(data)):
       mhr[i] = hrfilt.realtimeHR(data[i],fs)
208
209 for i in range(len(data2)):
       mhr2[i] = hrfilt.realtimeHR(data2[i],fs)
210
211
212 pyplot.figure(17)
pyplot.plot(np.linspace(0,len(data)/fs,len(data)),mhr)
214 pyplot.title('Momentary Heart Rate Plot from ECG.dat')
215 pyplot.xlabel('Time(s)')
pyplot.ylabel('Beats/Minute')
#pyplot.savefig('hr_fig17.eps', format='eps')
218
219 pyplot.figure(18)
pyplot.plot(np.linspace(0,len(data2)/fs,len(data2)),mhr2)
pyplot.title('Momentary Heart Rate Plot from einthoven II')
222 pyplot.xlabel('Time(s)')
223 pyplot.ylabel('Beats/Minute')
#pyplot.savefig('hr_fig18.eps', format='eps')
```

Listing 21: hr_detect.py

List of Figures

1	Ding Duffer Index Diagram	4
$\frac{1}{2}$	Ring Buffer Index Diagram	4 7
3	50 Hz Notch Filter IFFT	7
4	50 Hz Notch Filter IFFT (fixed) - Coefficients	8
5	DC Removal Filter Ideal Frequency Domain Plot	9
6	DC Removal Filter IFFT	10
7	DC Removal Filter IFFT (fixed) - Coefficients	10
8	Raw ECG from ECG.dat	12
9	Partly Raw ECG from ECG.dat	12
10	Raw ECG from Einthoven_ii Walking	13
11	Partly Raw ECG from Einthoven_ii Walking	13
12	Filtered ECG from ECG.dat	15 15
$\frac{12}{13}$		$\frac{15}{15}$
_	Partly ECG from ECG.dat	16 16
14	Filtered ECG from Einthoven_ii Walking	
15	Partly Filtered ECG from Einthoven_ii Walking	16
16	Raw ECG in Frequency Domain from ECG.dat	18
17	Filtered ECG from ECG.dat	20
18	Filtered ECG from Einthoven_ii Walking	21
19	1 ECG from ECG.dat	21
20	Reversed 1 ECG from ECG.dat	22
21	1 ECG from Einthoven_ii Walking	22
22	Reversed 1 ECG from Einthoven_ii Walking	23
23	Match Filter Result from ECG.dat	24
24	Match Filter Result from Einthoven_ii Walking	24
25	Squared Match Filter Result from ECG.dat	25
26	Squared Match Filter Result from Einthoven_ii Walking	26
27	Heart Beat Extraction using Threshold from ECG.dat	27
28	Heart Beat Extraction using Threshold from Einthoven_ii Walking	27
29	Heart Beat Extraction False 1s Deleted from ECG.dat	28
30	Heart Beat Extraction False 1s Deleted from Einthoven_ii Walking	29
31	Partly Heart Beat Extraction using Threshold from ECG.dat	29
32	Partly Heart Beat Extraction False 1s Deleted from ECG.dat	30
33	Momentary Heart Rate Plot from ECG.dat	31
34	Momentary Heart Rate Plot from Einthoven_ii Walking	31
35	Momentary Heart Rate Plot from shortecg.dat using filter class	
	implemented	34
36	Momentary Heart Rate Plot from shorteint.dat using filter class	
	implemented	34
37	self.counter Uses of Detecting Heart Beat from shortecg.dat	35
38	self.counter Uses of Detecting Heart Beat from shorteint.dat	35
39	Partly self.counter Uses of Detecting Heart Beat from shorteint.dat	36
40	Raw vs. Filtered data from Einthoven_ii Jogging	37
	~~~~	

# Listings

1	Initialise Constructor	2
2	Ring Buffer Function	3
3	dofilterPrint	4
4	unittest()	5
5	Import FIR_Filter Class	5
6	50 Hz Bandstop Coefficient	5
7	DC Filter Coefficient	8
8	Load .dat Files and Time Domain Plot	11
9	Filter operation and Filtered Time Domain Plot	13
10	Save .dat Files	17
11	Not Using Ring Buffer Version	17
12	Obtaining Coefficient for FIR filter	19
13	Matched Filter Implementation	23
14	Squaring the Results	24
15	Peak Threshold	26
16	Time Threshold	27
17	Momentary Heart Rate Calculation	30
18	Momentary Heart Rate Calculation	32
19	fir_filter.py	37
20	ecg_filter.py	39
21	hr_detect.py	42