

Implementation of iterative CT reconstruction

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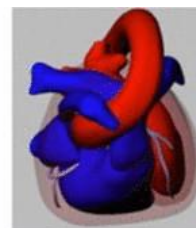


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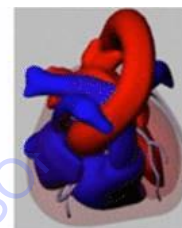
- **XCAT Phantom simulation**
 - *Geometry parameter setting*
 - *Sinogram generation with Poisson noise*
 - *Iterative reconstruction (SART, SQS)*
 - *Quadratic penalty for noise reduction*
- **Metal artifact correction (MAR)**
 - *Sinogram generation with metal artifact*
 - *Sinogram inpainting-based MAR*
- **Real patient data experiment**

XCAT phantom

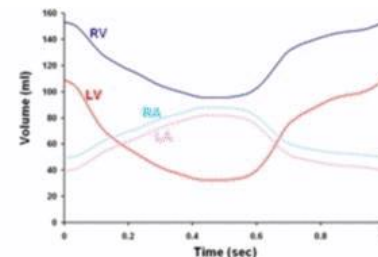
- Vector-based image generation
- Respiratory motion
- Cardiac motion
- Support various body conditions such as size, gender, etc.
- Used for CT and PET (3D and 4D)



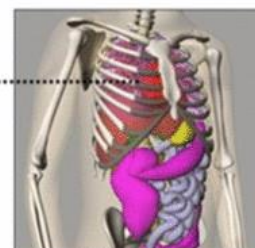
End-diastole



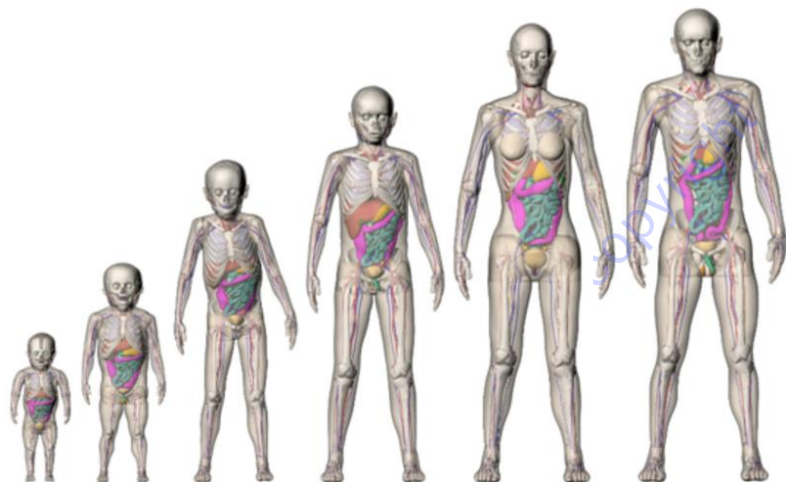
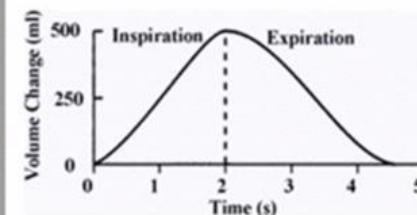
End-systole



End-expiration



End-inspiration



Segars, William Paul, et al. "Realistic CT simulation using the 4D XCAT phantom." Medical physics 35.8 (2008): 3800-3808.

Geometry of scanner

- **Helical CT:** whole-body



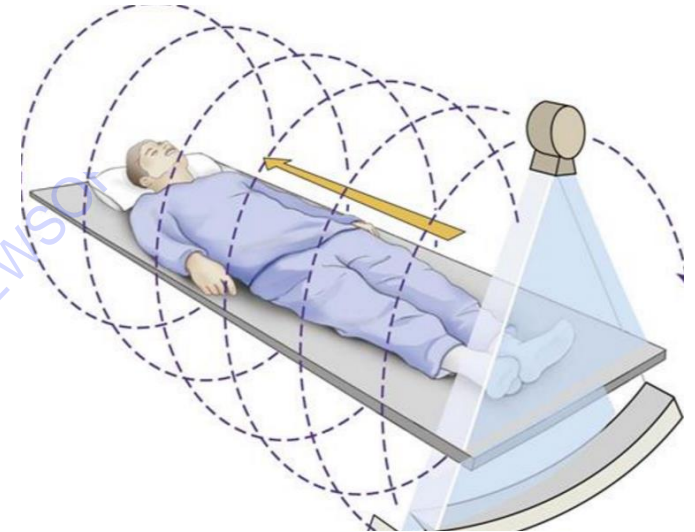
- **Slice rebinning for Helical CT**
 - 2D slice reconstruction

- **Cone-beam CT with flat detector:**
 - Dental, small animal, chest, brain...

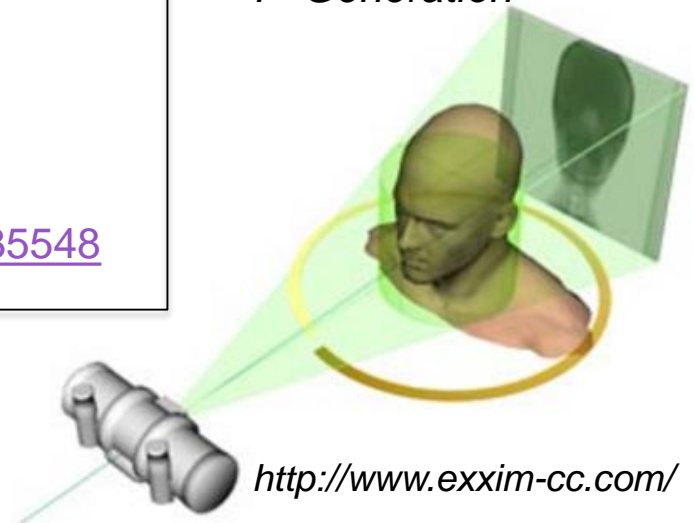
Free MATLAB Cone beam CT reconstruction code:

<http://www.mathworks.com/matlabcentral/fileexchange/35548>

3rd Generation



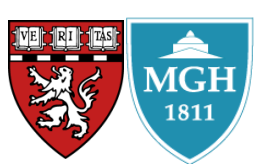
4th Generation



<http://www.exxim-cc.com/>

Initialization

- Requirements: Matlab + C compiler (OpenMP)
- Two zip files are given
 - PhantomExample_WinterSchool2017.zip
 - PatientExample_WinterSchool2017.zip
- Unzip “PhantomExample_WinterSchool2017.zip”
- Open “MeasurementGen.m” and run (F5)
 - If you see error message, please run CompileWindows/Linux/Mac
 - C compiler is required for MEX compilation
- If success, now you are ready
- Provide “projector” and “backprojector”



Geometry parameter setting

- Open “ParamSetting.m”

```
%% Parameter setting %%
```

```
param.nx = 256; % number of pixels  
param.ny = 256;
```

```
param.dx = 2; % mm  
param.dy = 2;
```

```
param.sx = param.nx*param.dx; % mm (whole size)  
param.sy = param.ny*param.dy; % mm
```

```
% X-ray source and detector setting
```

```
param.DSD = 1085.6; % Distance source to detector  
param.DSO = 595; % X-ray source to object axis distance
```

```
%The detector panel pixels (number of pixels)
```

```
param.nu = 736;
```

```
% Detector setting, cylindrical detector
```

```
param.du = 1.2858;  
param.fan_angle = param.du/param.DSD*180/3.141592*param.nu; % mm
```

```
% angle setting
```

```
param.dir = 1; % gantry rotating direction  
param.nview = 540; % number of views in one rotation (360 deg)  
param.dang = 360/param.nview;  
param.deg = [0:param.nview-1]*param.dang;  
param.deg = param.deg*param.dir;
```

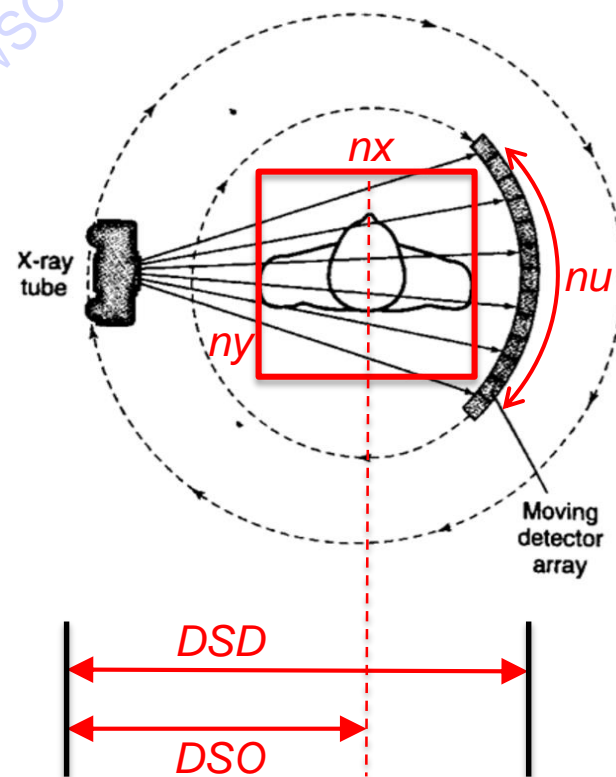
```
% filter='ram-lak' % high pass for sintetic images
```

```
param.filter='hamming'; % high pass for sintetic images
```

```
param.da = param.fan_angle/param.nu/180*3.141592; % rad
```

```
param.off_a = 0; % rad
```

nview: # of projections



Measurement generation

- Open “MeasurementGen.m”

```
load img_ref.mat
```

```
Slice = 1;
```

```
i0 = 8000;
```

← “i0” is a blank scan value

```
img_groundtruth = img_ref(:,:,Slice);
```

```
sino = CTproj_fan(img_groundtruth,param);
```

← projection to make a sinogram

```
sino_n = max(i0*exp(-sino),1);
```

```
sino_n = poissrnd(sino_n);
```

```
sino_n = -log(max(min(sino_n,i0),1)/i0);
```

← “poissrnd” function applies Poisson noise

$$y_e = i_0 e^{-\mu L}$$

$$y = -\log\left(\frac{y_e}{i_0}\right) = \mu L$$

Filtered back-projection (FBP)

- Two files: “filtering.m”, “CTbackproj_fan.m”

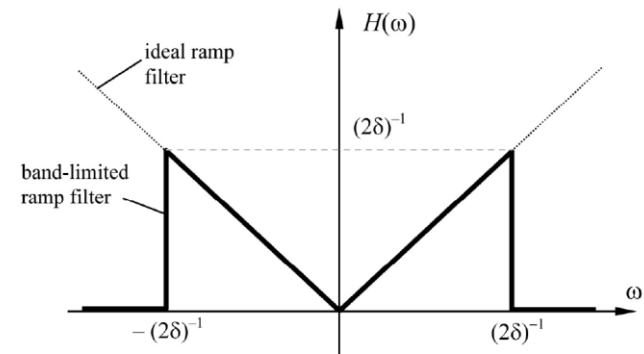
```
param.filter='hann';
```

```
sino_filt = filtering(sino_n,param);
```

```
img = max(CTbackproj_fan(sino_filt,param),0);
```

$$f(x, y) = \int_0^\pi d\theta \int_{-\infty}^{\infty} \boxed{P(\omega, \theta) |\omega| e^{j2\pi\omega t}} d\omega$$

(2) (1)



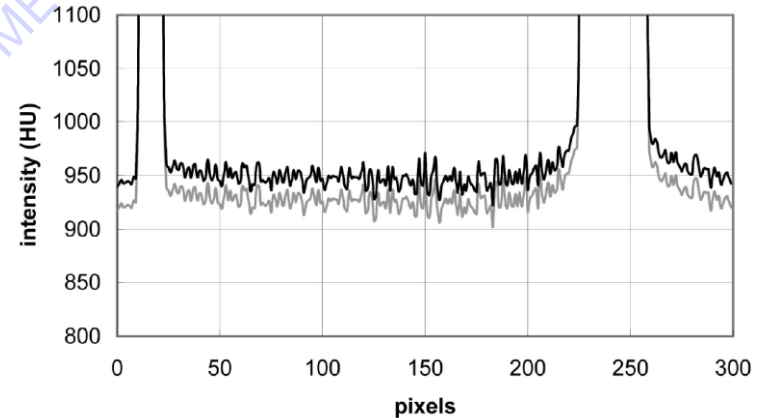
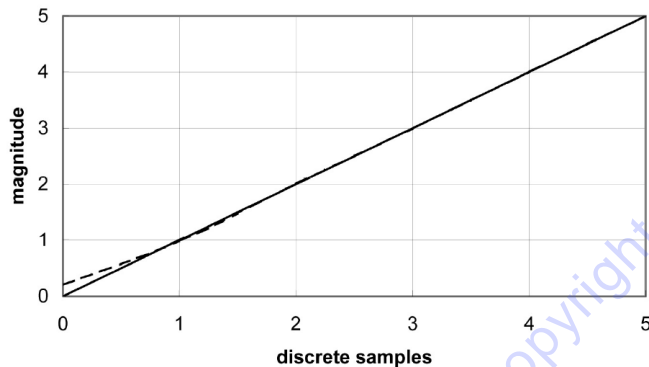
Filtered back-projection (FBP)

- Two files: “filtering.m”, “CTbackproj_fan.m”

```
param.filter='hann';
```

```
sino_filt = filtering(sino_n,param);
```

```
img = max(CTbackproj_fan(sino_filt,param),0);
```



Inaccurate ramp filter makes DC offsets

→ Digitalized ramp kernel is required

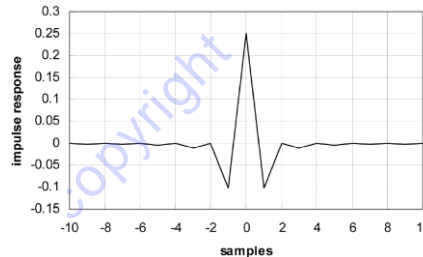
Filtered back-projection (FBP)

- Two files: “filtering.m”, “CTbackproj_fan.m”

```
param.filter='hann';  
  
sino_filt = filtering(sino_n,param);  
  
img = max(CTbackproj_fan(sino_filt,param),0);
```

❖ Solution

$$h(n\delta) = \begin{cases} \frac{1}{4\delta^2}, & n = 0, \\ 0, & n = \text{even}, \\ -\frac{1}{(n\pi\delta)^2}, & n = \text{odd}. \end{cases}$$



FFT



Resolution-
based
Ramp kernel

Additional low-pass filtering can be applied to reduce noise

Iterative reconstruction

- We define ...
 - Projection: A
 - Back-projection: A^T

$Ax : y = \text{CTproj_fan}(x, \text{param});$

Input: image, Output: sinogram

$A^T y : x = \text{CTbackproj_fan}(y, \text{param});$

Input: sinogram, Output: image

- Simultaneous algebraic reconstruction technique

```
%% SART
```

```
Norimg = CTbackproj_fan(CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
```

```
for iter = 1:50
```

```
    tic;
```

```
    % diff back projection
```

```
    sino_diff = CTproj_fan(img,param) - sino_n;
```

```
    Diffimg = CTbackproj_fan(sino_diff,param);
```

```
    % update
```

```
    img = max(img-Diffimg./Norimg,0);
```

```
    img(isnan(img))=0;
```

```
    figure(11); imagesc(max(img,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['iter - ',num2str(iter)]);
```

```
    pause(0.1);
```

```
    exetime = toc;
```

```
    disp([num2str(iter),' - iteration done.. ']/ Exe. time (sec) : ', num2str(exetime)]);
```

```
end
```

- Simultaneous algebraic reconstruction technique

$$x^{n+1} = x^n - \frac{A^T (Ax^n - y)}{A^T A}$$

(0)

$$A^T A = A^T A I, \quad I = \text{image of ones}$$

We can pre-calculate the normalization term

```
Norimg = CTbackproj_fan(CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
```

$$y = -\log(y_e/i_0)$$

- Simultaneous algebraic reconstruction technique

$$x^{n+1} = x^n - \frac{A^T (Ax^n - y)}{A^T A}$$

- (1) `sino_diff = CTproj_fan(img,param) - sino_n;`
(2) `Diffimg = CTbackproj_fan(sino_diff,param);`

SART

- Simultaneous algebraic reconstruction technique

$$(4) \quad x^{n+1} = x^n - \frac{A^T (Ax^n - y)}{A^T A} \quad (3)$$

% update

$$(4) \quad \text{img} = \max(\text{img} - \frac{\text{Diffimg}}{\text{Norimg}}, 0); \quad (3)$$

SQS (separable quadratic surrogate)

Precompute and store: $d_j^* = \sum_{i=1}^N a_{ij} \gamma_i (y_i - r_i)^2 / y_i$, where $\gamma_i = \sum_j a_{ij}$

for each subset Compute: \hat{l}_i, \hat{h}_i as in (19) in table 1

Update:

$$\mu_j := \left[\mu_j - \frac{M \sum_{i \in S_m} a_{ij} \hat{h}_i}{d_j^*} \right]_+ . \quad \hat{l}_i = \sum_{j=1}^p a_{ij} \hat{\mu}_j \quad \hat{h}_i = \left(\frac{y_i}{b_i e^{-\hat{l}_i} + r_i} - 1 \right) b_i e^{-\hat{l}_i}$$

end

Scatter and noise

$$x^{n+1} = x^n - \frac{A^T \left(\frac{y_e}{i_0 e^{-Ax^n} + r} - 1 \right) i_0 e^{-Ax^n}}{A^T \frac{y_e - r}{y_e} A}$$

SQS (separable quadratic surrogate)

$$x^{n+1} = x^n - \frac{A^T \left(\frac{y_e}{i_0 e^{-Ax^n} + r} - 1 \right) i_0 e^{-Ax^n}}{A^T \frac{y_e - r}{y_e} A}$$

Pre-corrected
Scatter and noise

$$\approx x^n - \frac{A^T \left(\frac{y_e}{i_0 e^{-Ax^n}} - 1 \right) i_0 e^{-Ax^n}}{A^T y_e A}$$

MLTR: *maximum likelihood transmission*

SQS (separable quadratic surrogate)

$$x^{n+1} = x^n - \frac{A^T \left(\frac{y_e}{i_0 e^{-Ax^n}} - 1 \right) i_0 e^{-Ax^n}}{A^T y_e A}$$

$A^T y_e A$: Pre-calculation

```
Noring = CTbackproj_fan(sino_exp.*CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
```

Ax : Projection

$A^T(\cdot)$: Backprojection of residual

SQS (*separable quadratic surrogate*)

```
%% SQS
```

```
sino_exp = i0*exp(-sino_n);
```

```
Norimg = CTbackproj_fan(sino_exp.*CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
```

```
for iter = 1:50
```

```
tic;
```

```
% diff back projection
```

```
sino_tmp = i0*exp(-CTproj_fan(img,param) );
```

```
sino_diff = (sino_exp./sino_tmp - 1) .* sino_tmp;
```

```
sino_diff(isnan(sino_diff)) = 0;
```

```
sino_diff(isinf(sino_diff)) = 0;
```

```
Diffimg = CTbackproj_fan(sino_diff,param);
```

```
% update
```

```
img = max(img-Diffimg./Norimg,0);
```

```
img(isnan(img))=0;
```

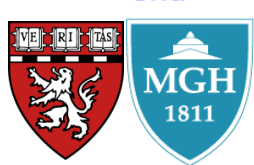
```
figure(11); imagesc(max(img,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['iter - ',num2str(iter)]);
```

```
pause(0.1);
```

```
exetime = toc;
```

```
disp([num2str(iter),' - iteration done.. ', '/ Exe. time (sec) : ', num2str(exetime)]);
```

```
end
```



Quadratic penalty

$$R(x) = \frac{1}{2} \sum_j^{N_v} \sum_{j' \in \Omega} \rho_{jj'} (x_j - x_{j'})^2$$

$$\dot{R}(x_j) = \sum_{j' \in \Omega} \rho_{jj'} (x_j - x_{j'})$$

$$\ddot{R}(x_j) = \sum_{j' \in \Omega} \rho_{jj'} = 1$$

➤ quadpenalty(img, 1) = $\dot{R}(x_j)$

Iterative recon + quadratic penalty

- SART + quadratic penalty

$$x^{n+1} = x^n - \frac{A^T (Ax^n - y) + \beta \dot{R}(x^n)}{A^T A + \beta \ddot{R}(x^n)}$$

- SQS + quadratic penalty

$$x^{n+1} = x^n - \frac{A^T \left\{ \left(\frac{y_e}{i_0 e^{-Ax^n}} - 1 \right) i_0 e^{-Ax^n} \right\} + \beta \dot{R}(x^n)}{A^T y_e A + \beta \ddot{R}(x^n)}$$

SART with Quadratic penalty

```
Norimg = CTbackproj_fan(CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
Beta = 0.03.*Norimg;

for iter = 1:50

    tic;
    % diff back projection
    sino_diff = CTproj_fan(img,param) - sino_n;
    Diffimg = CTbackproj_fan(sino_diff,param);

    % Quadratic penalty
    img_quad = quadpenalty(img,1);

    % update
    img = max(img-(Diffimg+Beta.*img_quad)./(Norimg+Beta),0);
    img(isnan(img))=0;

    figure(11); imagesc(max(img,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['iter - ',num2str(iter)]);
    pause(0.1);
    exetime = toc;

    disp([num2str(iter),' - iteration done.. ','/ Exe. time (sec) : ', num2str(exetime)]);
end
```


SQS with Quadratic penalty

```
%% SQS
```

```
sino_exp = i0*exp(-sino_n);
```

```
Norimg = CTbackproj_fan(sino_exp.*CTproj_fan(ones(param.nx,param.ny,'single'),param),param);
```

```
Beta = 0.03.*Norimg;
```

```
for iter = 1:50
```

```
tic;
```

```
% diff back projection
```

```
sino_tmp = i0*exp(-CTproj_fan(img,param) );
```

```
sino_diff = (sino_exp./sino_tmp - 1) .* sino_tmp;
```

```
sino_diff(isnan(sino_diff)) = 0;
```

```
sino_diff(isinf(sino_diff)) = 0;
```

```
Diffimg = CTbackproj_fan(sino_diff,param);
```

```
% Quadratic penalty
```

```
img_quad = quadpenalty(img,1);
```

```
% update
```

```
img = max(img-(Diffimg+Beta.*img_quad)./(Norimg+Beta),0);
```

```
img(isnan(img))=0;
```

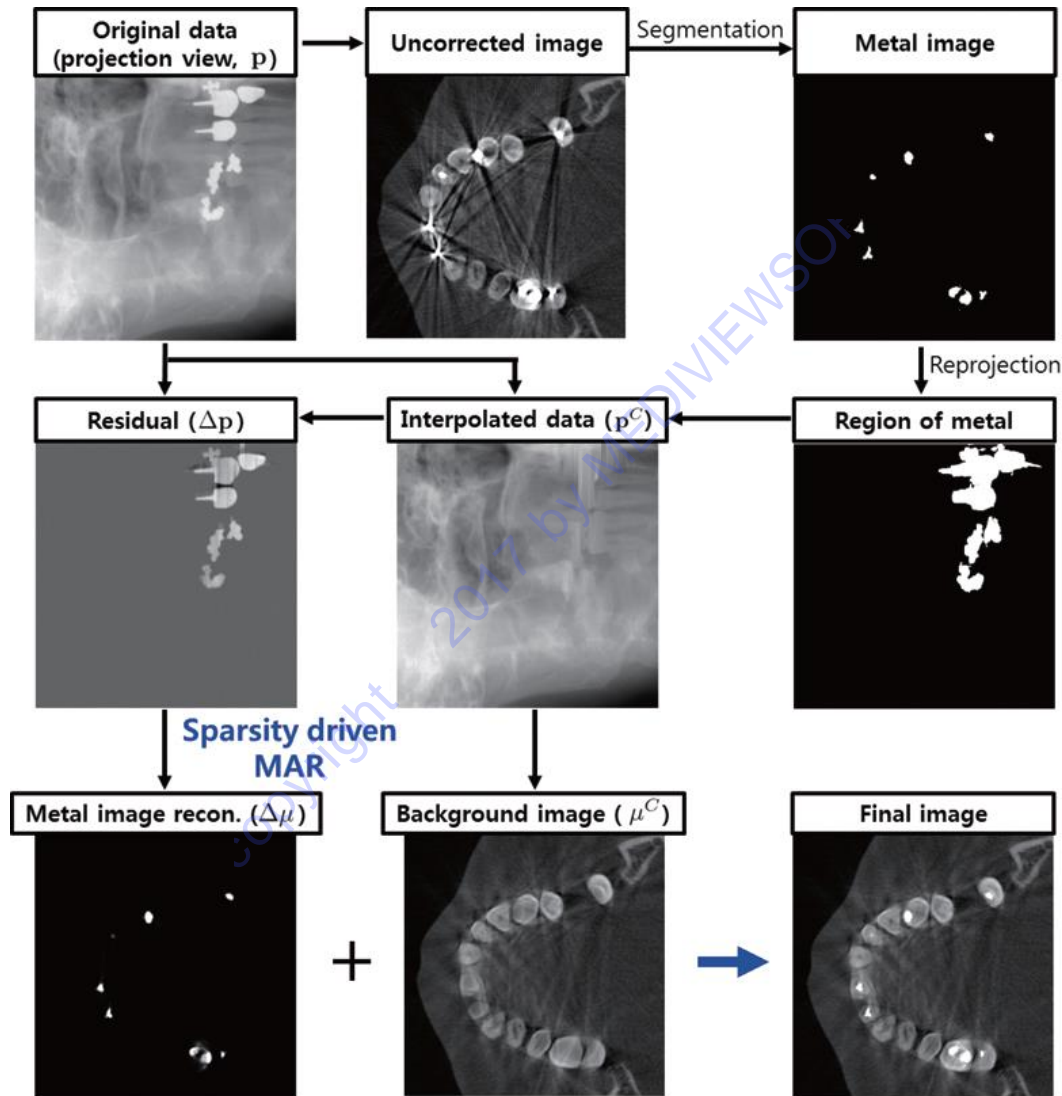
```
figure(11); imagesc(max(img,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['iter - ',num2str(iter)]);
```

```
pause(0.1);
```

```
exetime = toc;
```

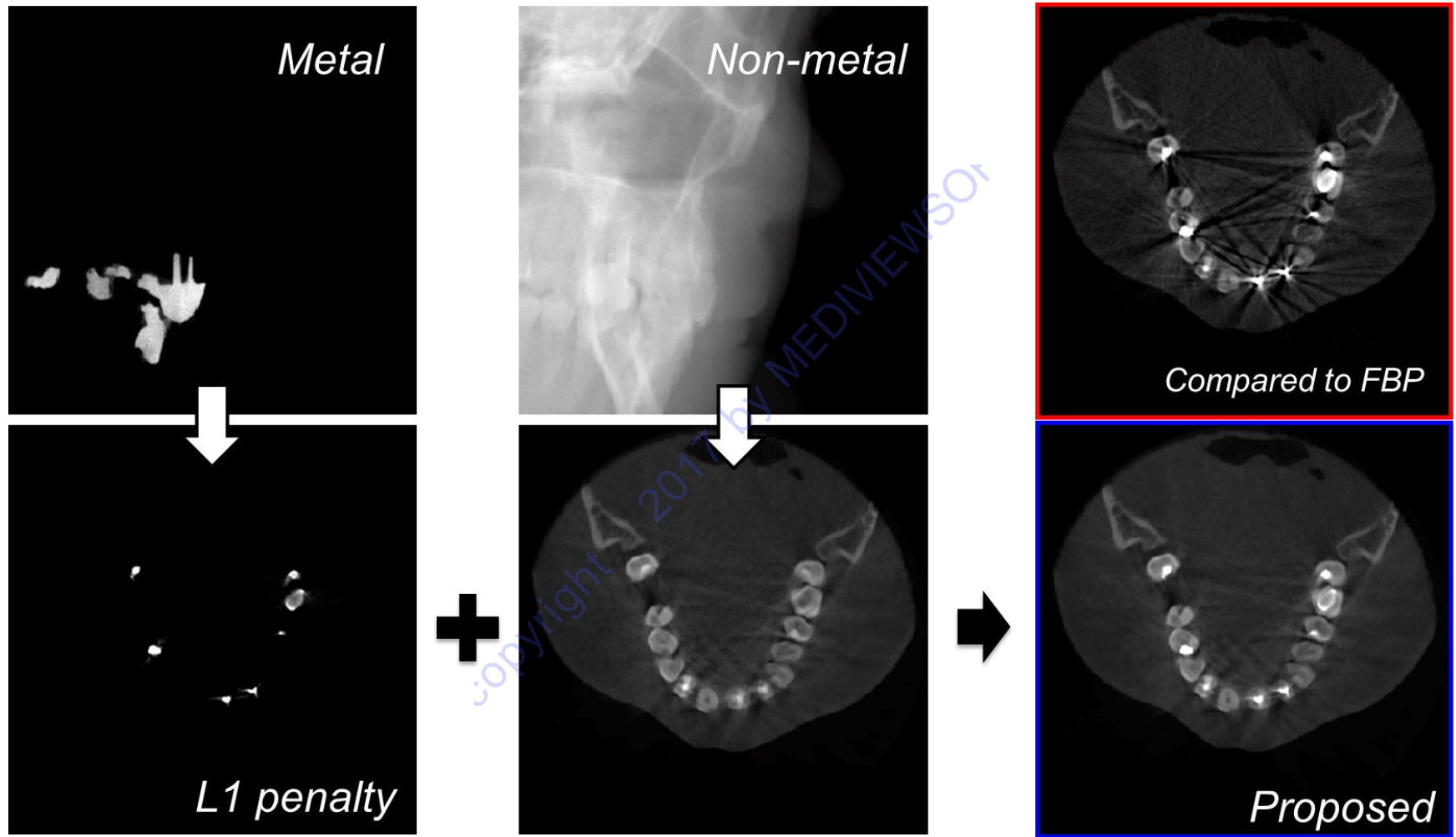
```
disp([num2str(iter),' - iteration done.. ','/ Exe. time (sec) : ', num2str(exetime)]);
```

Metal artifact reduction flow chart



J. Choi, K. Kim, M. W. Kim, W. Seong and J. C. Ye, Sparsity Driven Metal Part Reconstruction for Artifact Removal in Dental CT, Journal of X-ray Science and Technology, vol. 19, pp. 457-475, October 2011.

Metal artifact reduction flow chart



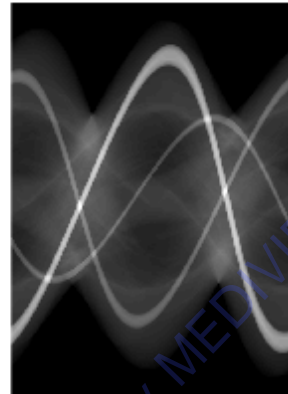
Metal artifact sinogram generation

```
nMetal = 3;
cx = [35, 105, 208];
cy = [129, 81, 119];
intensity = [ 0.3, 0.3, 0.2];
r = [7, 3, 5];
for id = 1:nMetal
    for ix=cx(id)-r(id):cx(id)+r(id)
        for iy = cy(id)-r(id):cy(id)+r(id)
            if sqrt((ix-cx(id))^2+(iy-cy(id))^2)<=r(id)
                img_groundtruth(ix,iy) = intensity(id)
            end
        end
    end
end

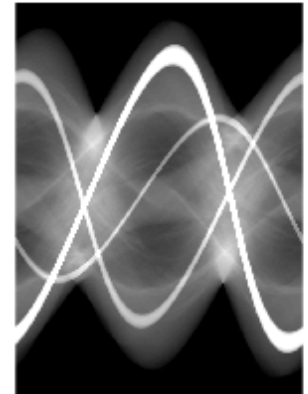
sino = CTproj_fan(img_groundtruth,param);

sino_n = max(i0*exp(-sino),1);
% sino_n = poissrnd(sino_n);
sino_n = -log(max(min(sino_n,i0),1)/i0);
```

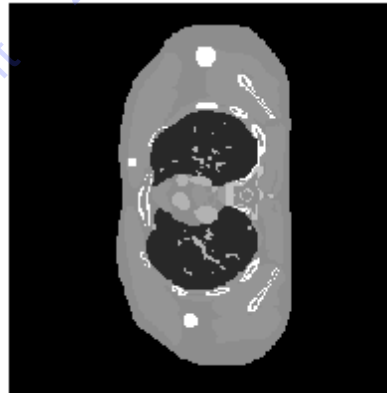
Noiseless



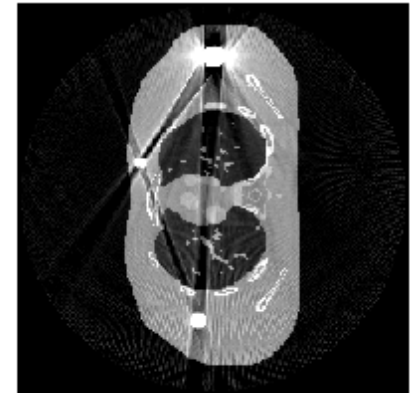
Metal Artifact



Noiseless



Metal Artifact



Initial FDK

%% 1. filtered backprojection (initialization)

```
param.filter='hann';
```

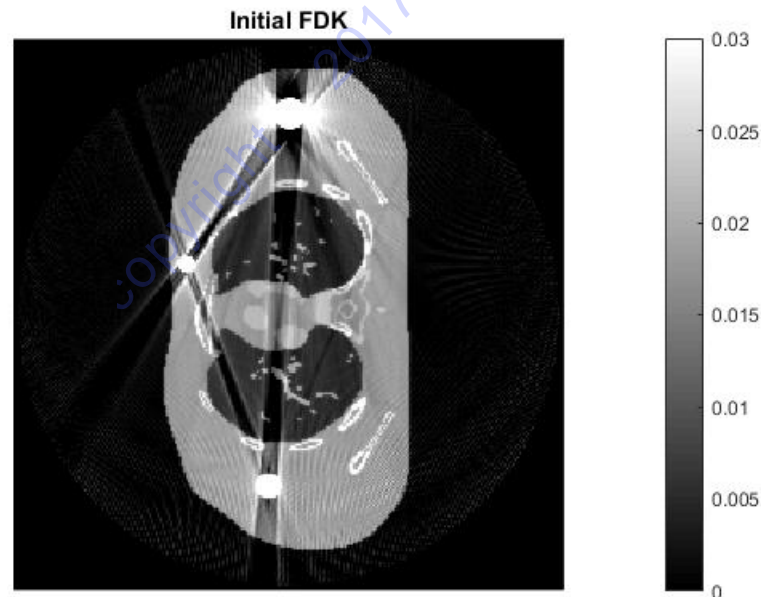
```
tic;
```

```
sino_filt = filtering(sino_n,param);
```

```
imgFDK = max(CTbackproj_fan(sino_filt,param),0);
```

```
toc;
```

```
figure(1); imagesc(imgFDK,[ 0 0.03]); axis off; axis equal; colormap gray; colorbar; title('Initial FDK');  
pause(0.1);
```



Mask of metallic part

%% 2. Metal object reprojection to make a mask

```
Metal_Threshold = 0.1;  
img_metal = zeros(param.nx, param.ny, 'single');  
img_metal(imgFDK>Metal_Threshold) = 1;  
  
sino_mask = CTproj_fan(img_metal, param);  
sino_mask(sino_mask>0) = 1;  
  
figure(2); imagesc(sino_mask); axis off; axis equal; colormap gray; colorbar; title('Mask Sinogram');  
pause(0.1);
```

Mask Sinogram



Sinogram inpainting

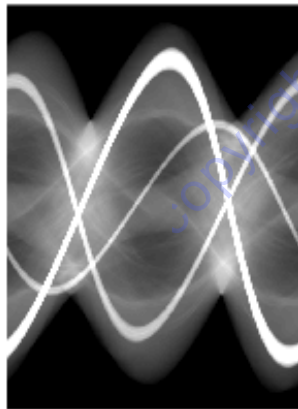
%% 3. inpainting

```
sino_nonMetal = sino_n;  
sino_nonMetal(sino_mask == 1) = NaN;
```

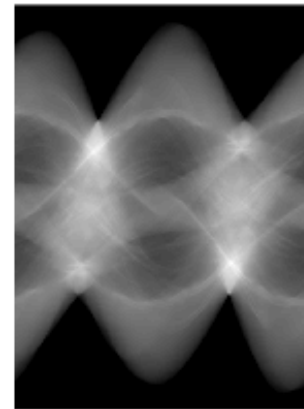
```
sino_nonMetal = inpaintn(sino_nonMetal,300);
```

```
figure(3);  
subplot(1,2,1); imagesc(sino_n); axis off; axis equal; colormap gray; colorbar; title('Orig Sinogram');  
subplot(1,2,2); imagesc(sino_nonMetal); axis off; axis equal; colormap gray; colorbar; title('inpainting Sinogram');  
pause(0.1);
```

Orig Sinogram



inpainting Sinogram



Reconstruction of non-metal object

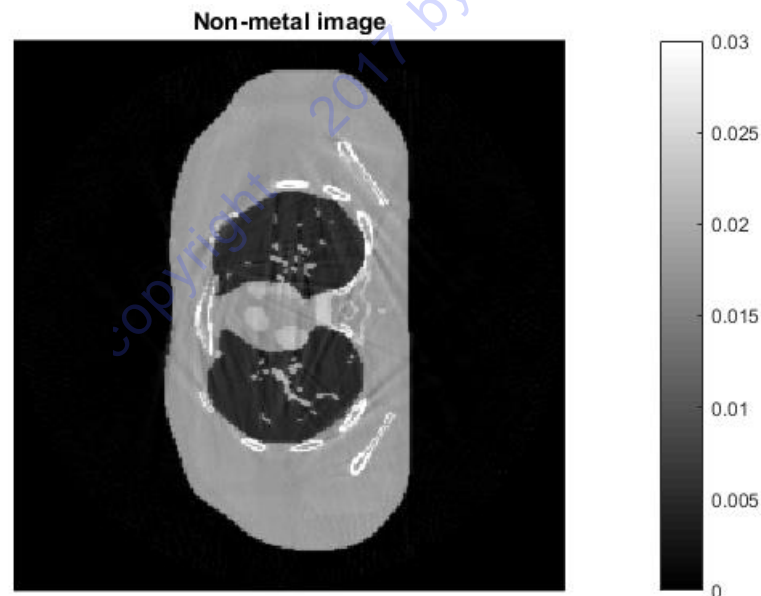
%% 4. reconstruction of non-metal part

```
param.filter='hann';
```

```
sino_filt = filtering(sino_nonMetal,param);
```

```
img_nonMetal = max(CTbackproj_fan(sino_filt,param),0);
```

```
figure(4); imagesc(img_nonMetal,[ 0 0.03]); axis off; axis equal; colormap gray; colorbar; title('Non-metal image');  
pause(0.1);
```



L1-based metal object recon.

%% Metal reconstruction (FDK -> SART+L1)

```
sino_Metal = sino_n - CTproj_fan(img_nonMetal,param);  
sino_filt = filtering(sino_Metal,param);  
img_Metal = max(CTbackproj_fan(sino_filt,param),0);
```

```
Norimg = CTbackproj_fan(CTproj_fan(ones(param.nx,param.ny,'single'),param),param);  
Beta = 0.5.*Norimg;  
gamma = 0.01;
```

```
for iter = 1:50
```

```
tic;
```

```
% diff back projection
```

```
sino_diff = CTproj_fan(img_Metal,param) - sino_Metal;  
Diffimg = CTbackproj_fan(sino_diff,param);
```

```
% L1 penalty: soft thresholding
```

```
img_L1 = img_Metal - max(img_Metal-gamma,0);
```

```
% update
```

```
img_Metal = max(img_Metal-(Diffimg+Beta.*img_L1)./(Norimg+Beta),0);  
img_Metal(isnan(img_Metal))=0;
```

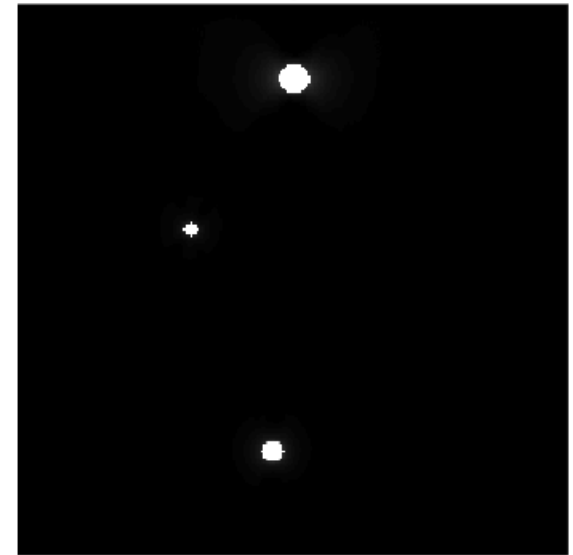
```
figure(5); imagesc(max(img_Metal,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['Metal image iter - ',num2str(iter)]);  
pause(0.01);  
exetime = toc;
```

```
disp([num2str(iter),' - iteration done.. ']/ Exe. time (sec) : ', num2str(exetime)]);
```

```
end
```

$$\min_{x_m} \frac{1}{2} \|y_m - Ax_m\|_2^2 + \lambda \|x_m\|_1$$

Metal image iter - 50



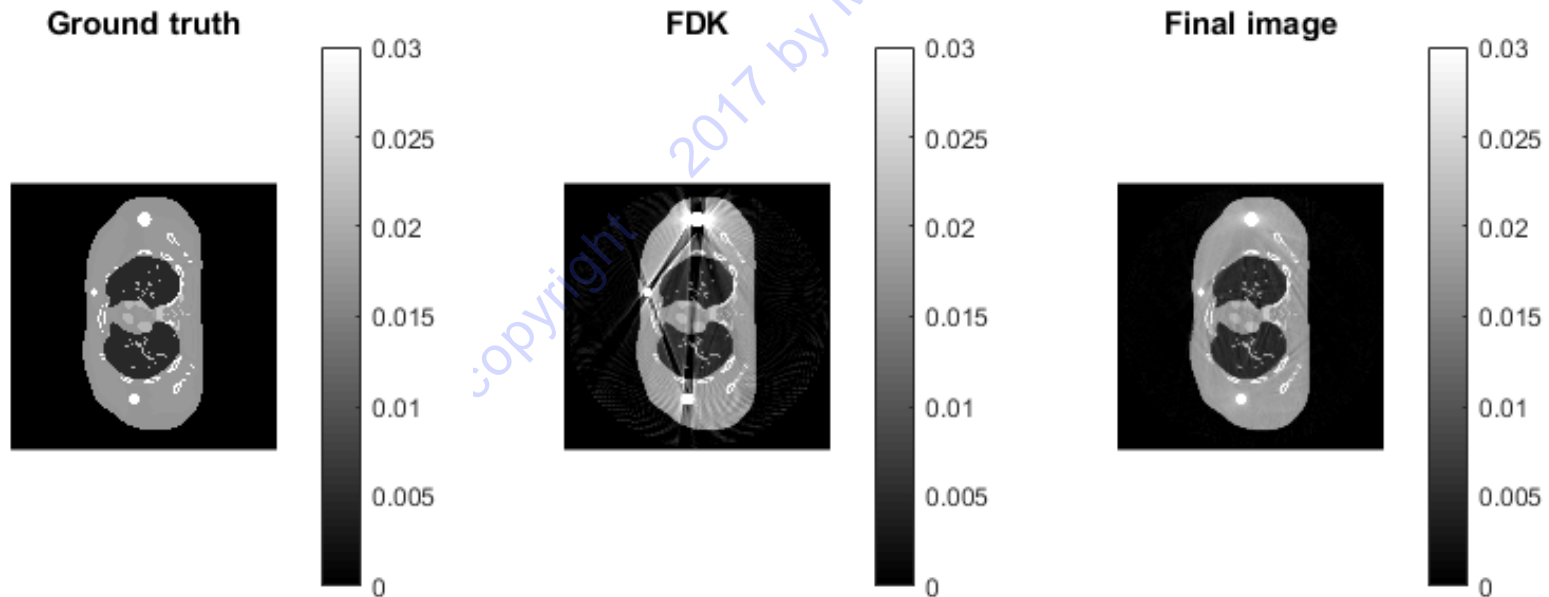
K. Kim, J. C. Ye, G. E. Fakhri and Q. Li, Metal artifact reduction using l1 and non-local penalties with iterative sinogram correction, The Third International Conference on Image Formation in X-Ray Computed Tomography, Salt Lake City, Utah, USA, June, 2014

Sum of non-metal and metal images

%% Final image

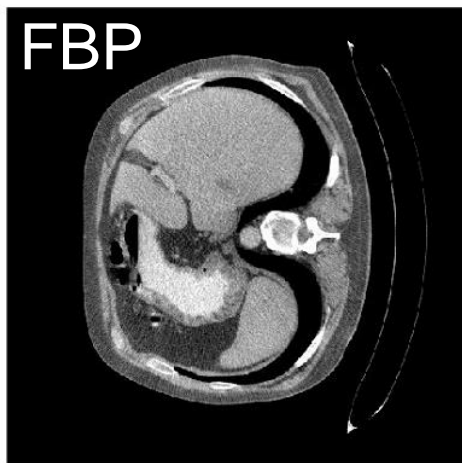
```
img = img_nonMetal+img_Metal;
```

```
figure(6);  
subplot(1,3,1); imagesc(max(img_groundtruth,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['Ground truth']);  
subplot(1,3,2); imagesc(max(imgFDK,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['FDK']);  
subplot(1,3,3); imagesc(max(img,0),[0 0.03]); axis off; axis equal; colormap gray; colorbar; title(['Final image']);  
pause(0.1);
```

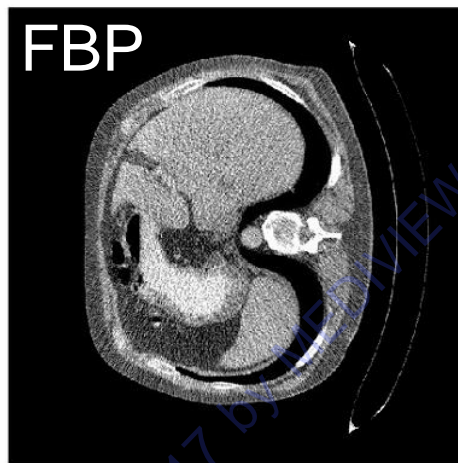


Patient data

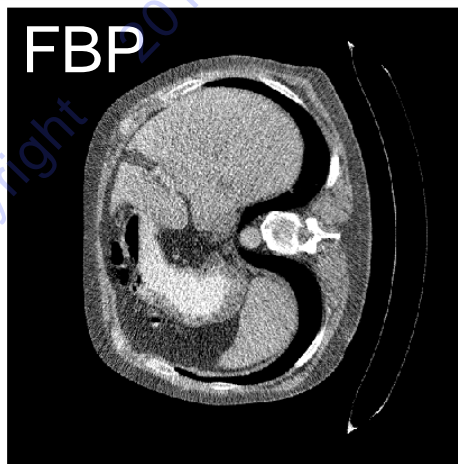
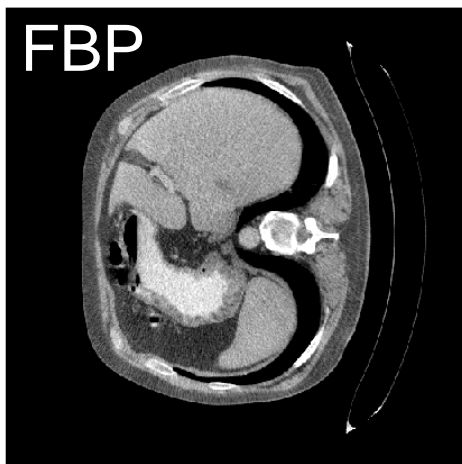
Regular dose



Quarter dose



Iterative recon



Thank you for your attention!

