

Breaking Speed Limits with Simultaneous Ultra-Fast MRI Reconstruction and Tissue Segmentation



Paper #239



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Disclosure

I have no financial interests or relationships to disclose with regard to the subject matter of this presentation.

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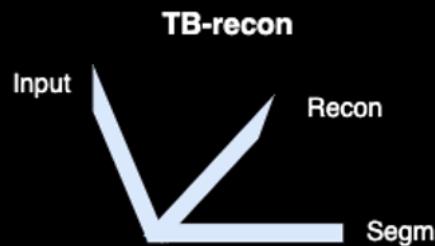
Deep Learning in Magnetic Resonance Imaging (MRI)

- Long scanning time is the **main** limitation of MRI
- We devised a DL framework for **MRI reconstruction and segmentation** from highly undersampled MRIs
- We bridged image reconstruction and analysis by proposing a **task-based** reconstruction approach

Input: 1.5× AF

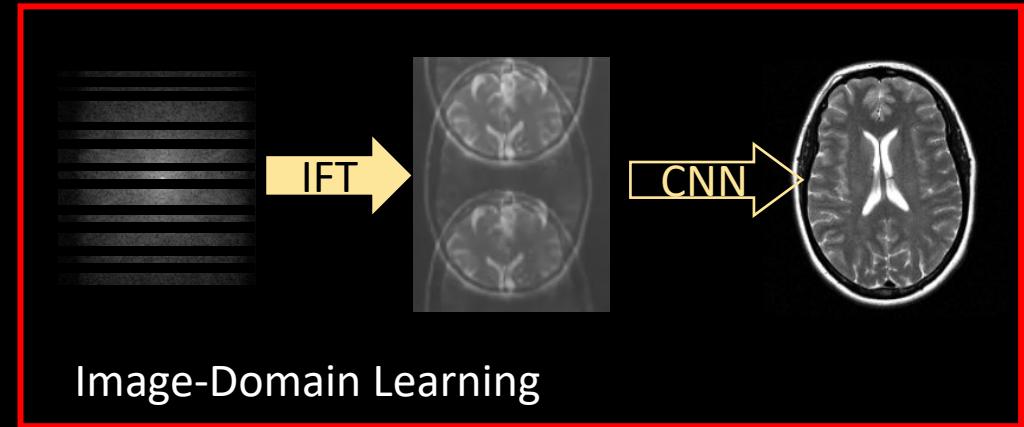


Reconstruction + Segmentation



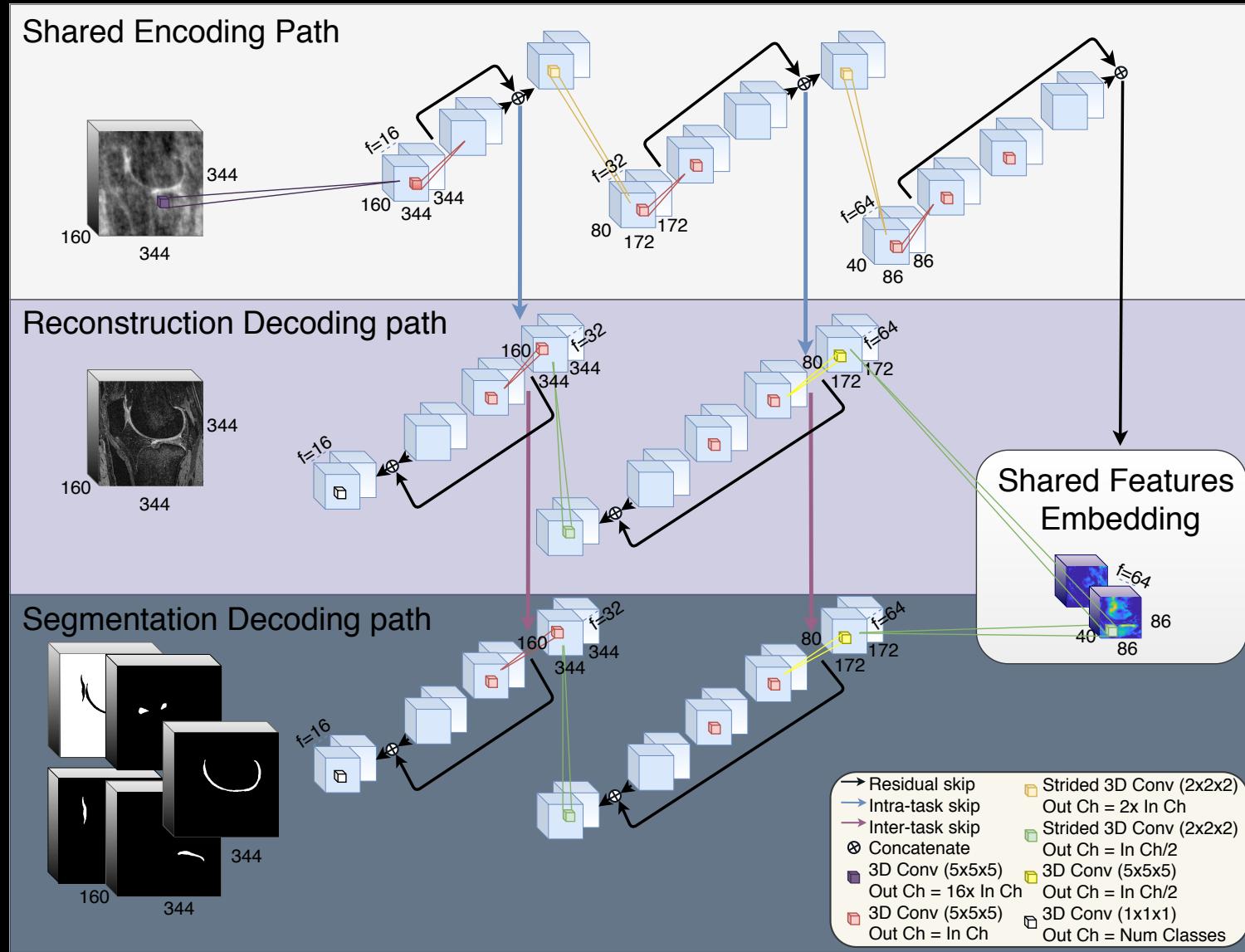
Hypotheses:

- Reconstruction in the image-domain provides higher data **interpretability** over k-space
- Reconstruction and segmentation are similar and related tasks

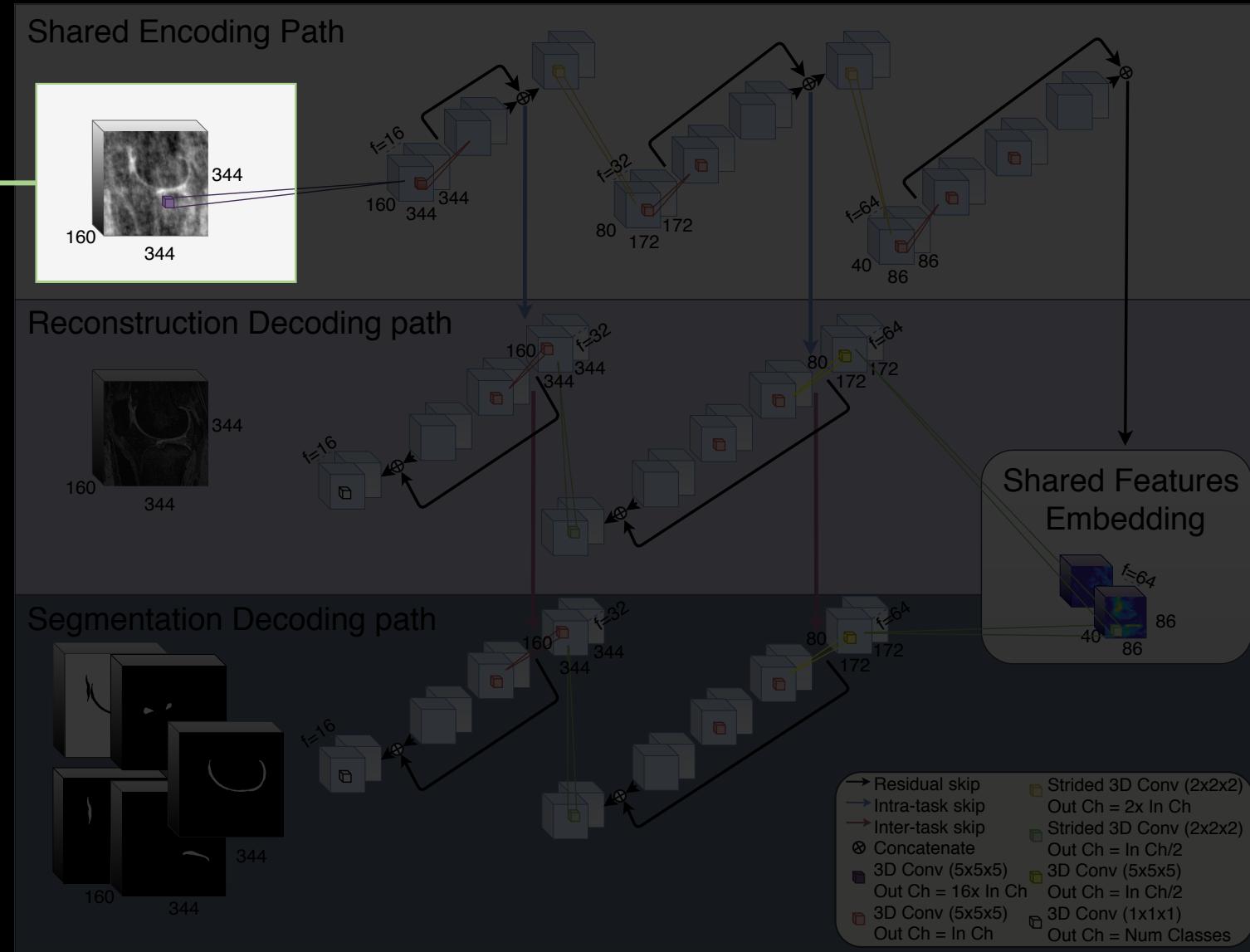


Simultaneous segmentation and image reconstruction

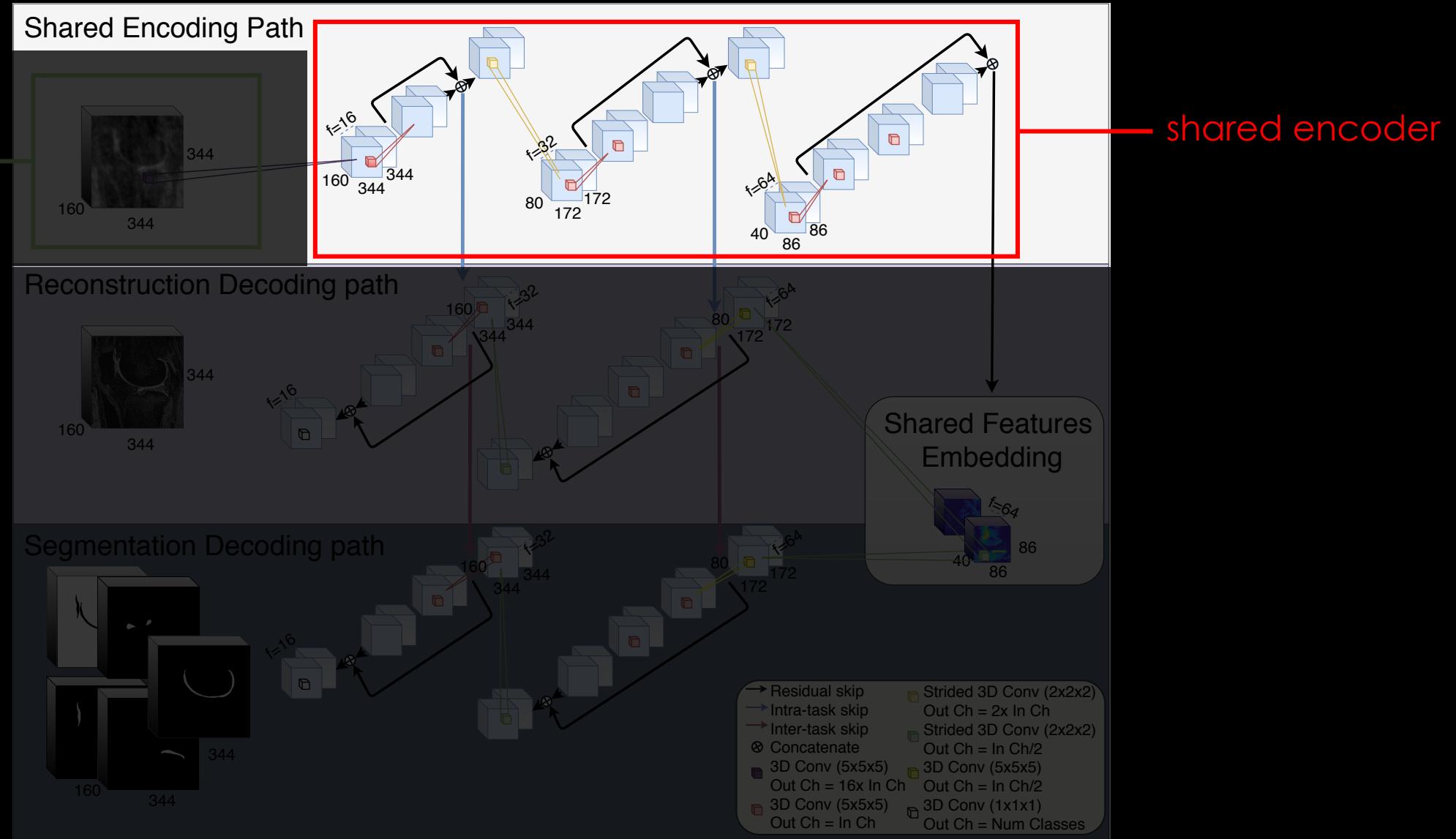
Proposed approach: Task-based image reconstruction: TB-recon



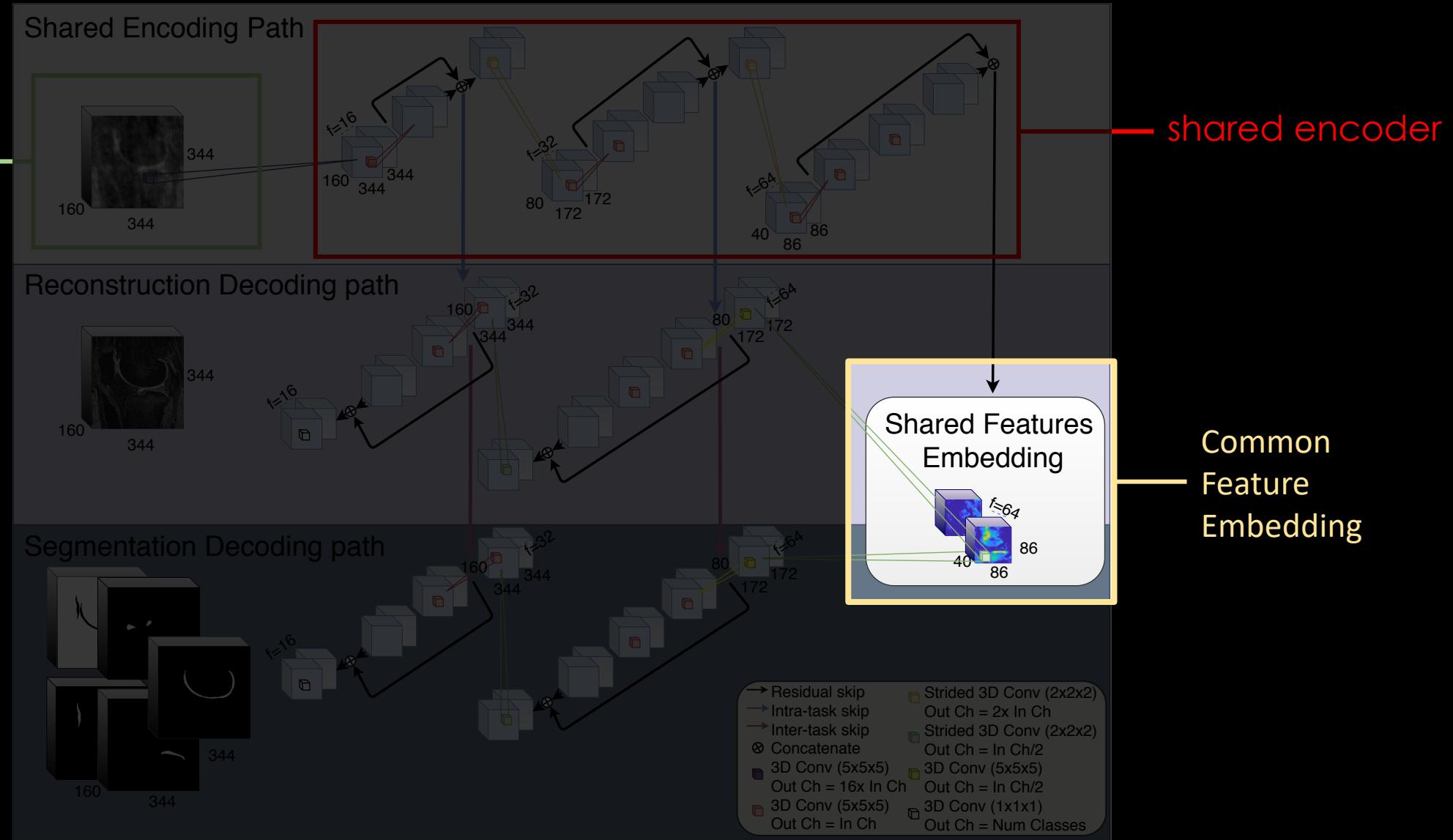
Input:
zero-filled MRI



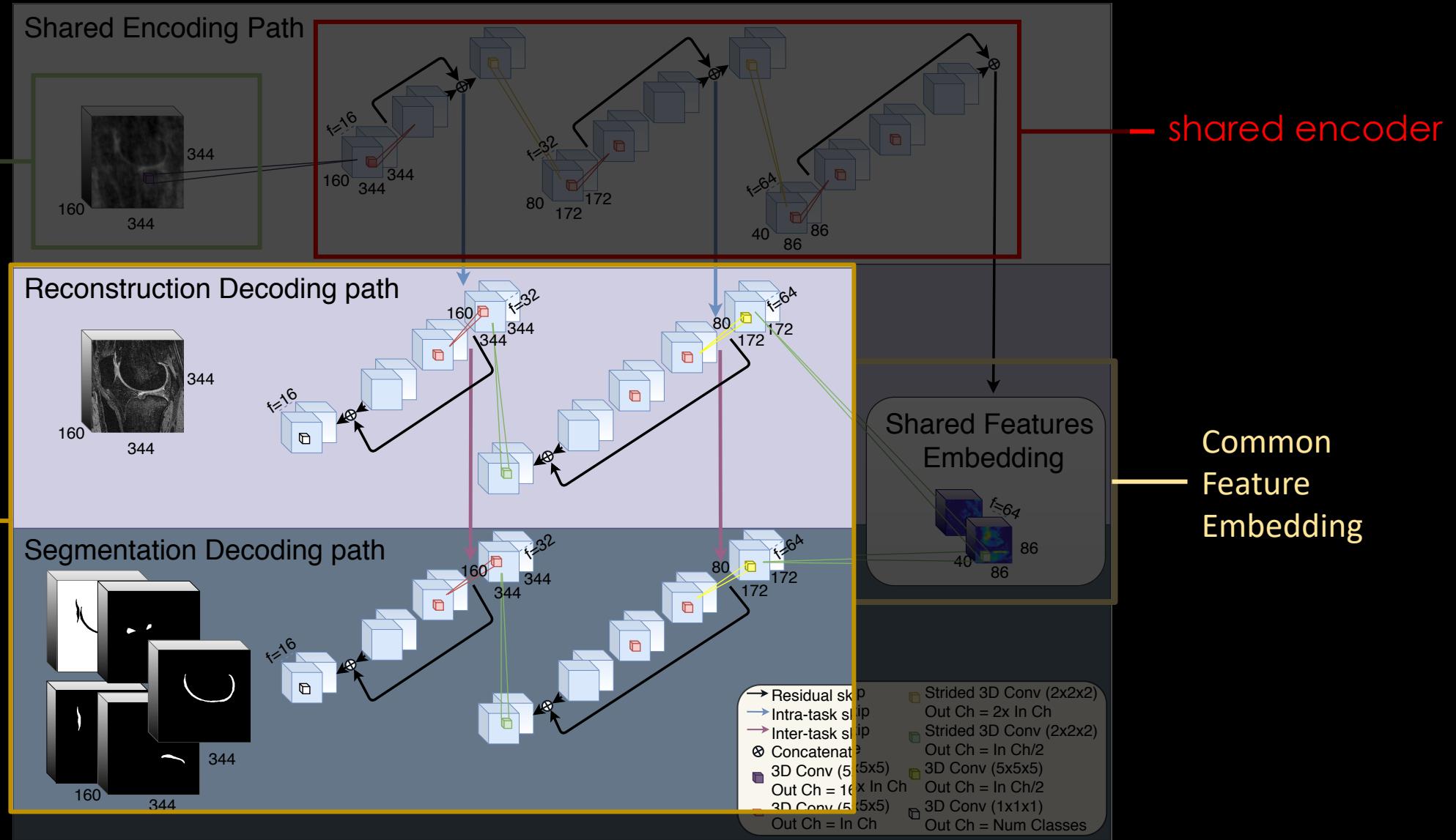
Input:
zero-filled MRI



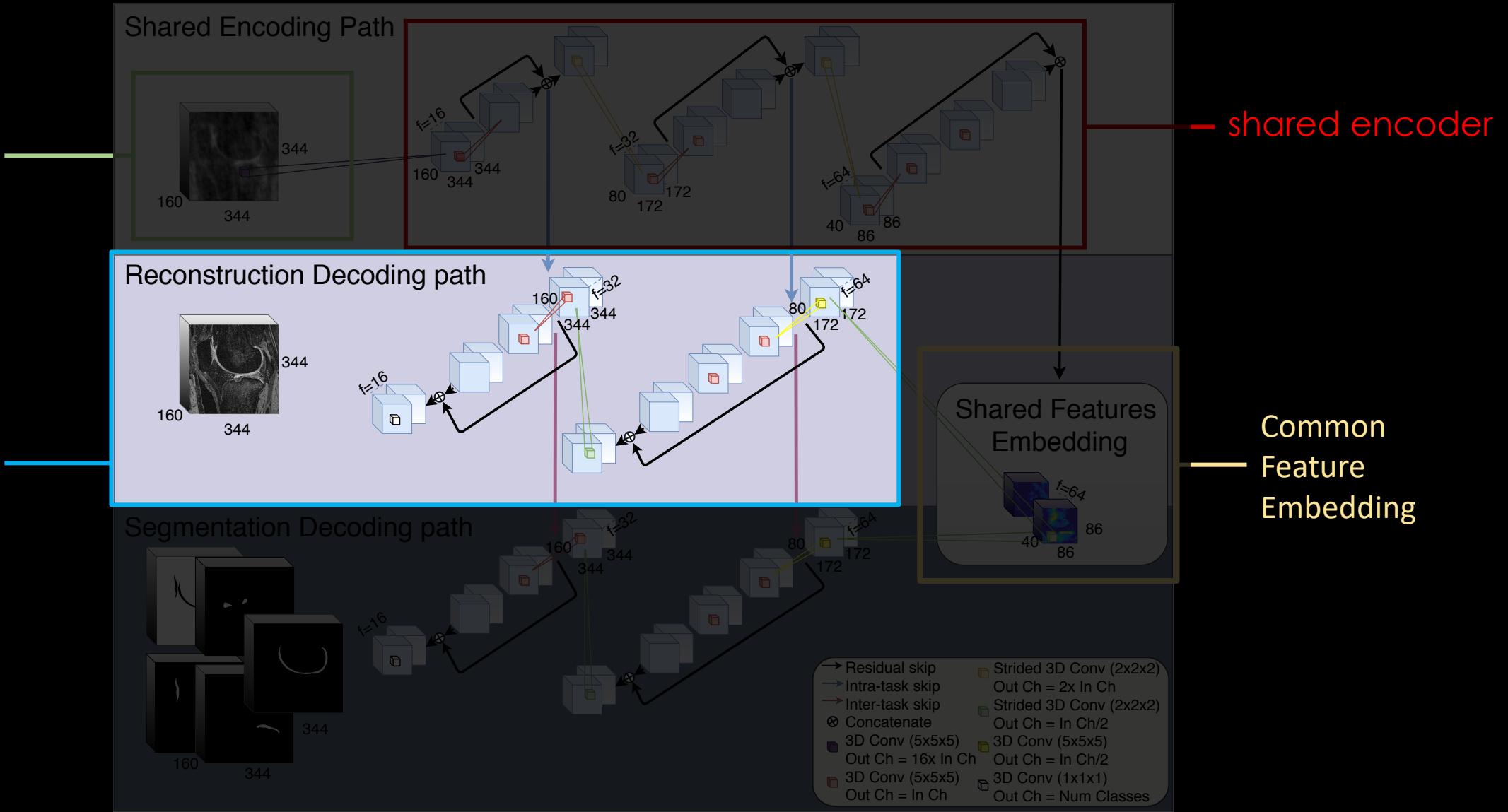
Input:
zero-filled MRI



Input:
zero-filled MRI



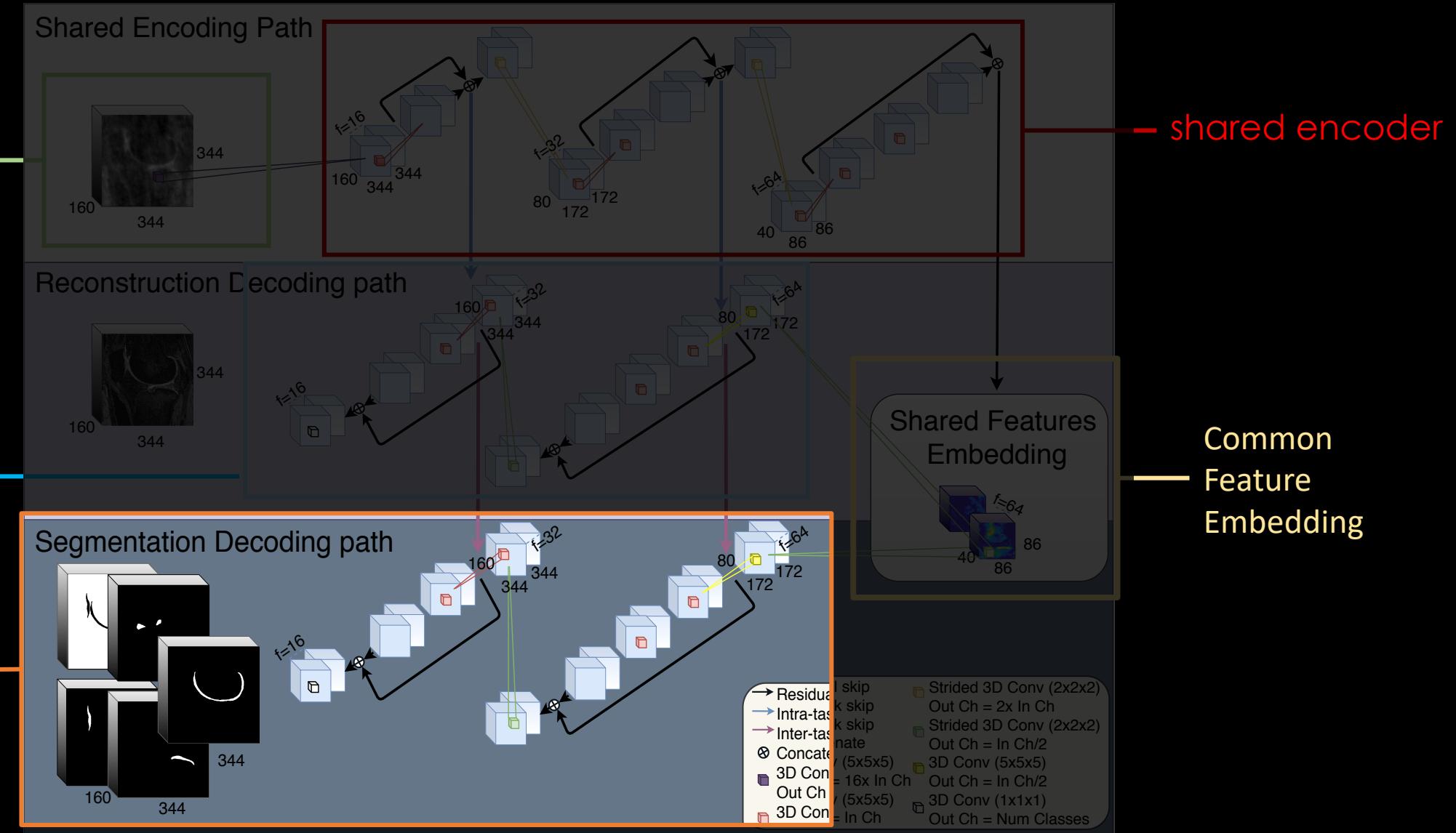
Input:
zero-filled MRI



Input:
zero-filled MRI

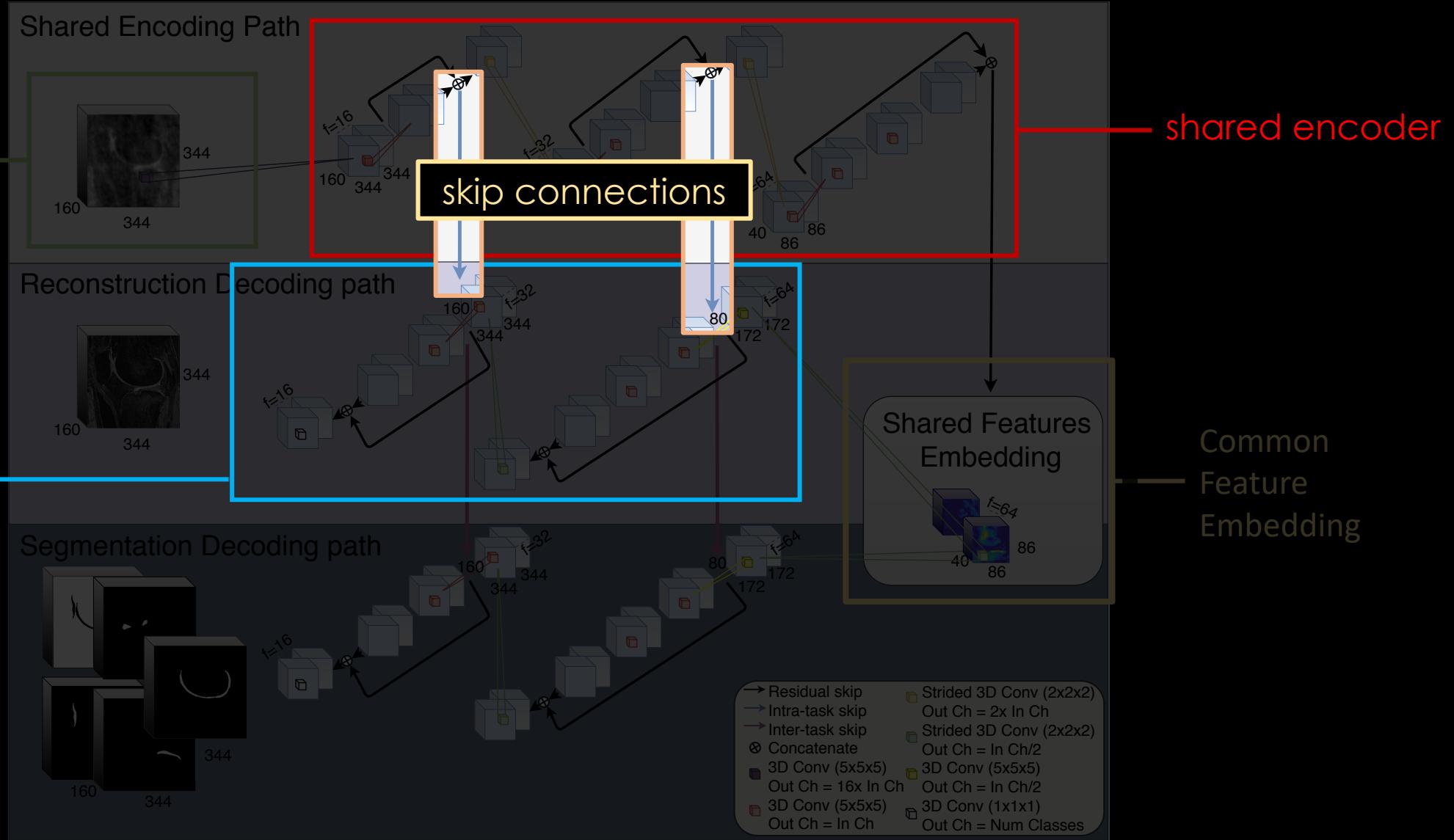
reconstruction
decoder

segmentation
decoder



Input:
zero-filled MRI

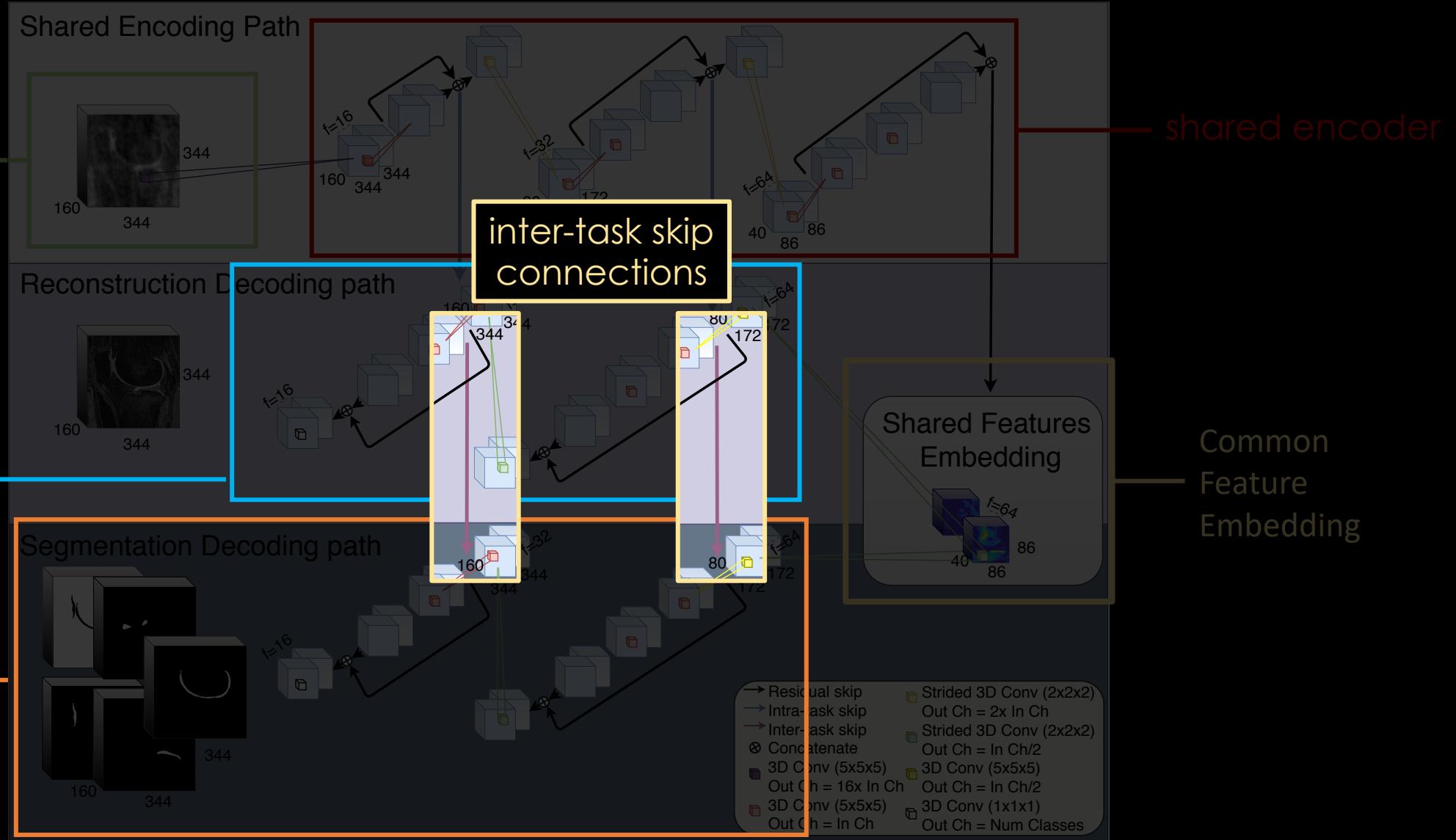
reconstruction
decoder
output: linear



Input:
zero-filled MRI

reconstruction
decoder

segmentation
decoder
output: softmax
activation



Input:
zero-filled MRI



End-to-end network training

- Undersampled zero-filled MRI denoising and tissue segmentation
- A multi-task loss is minimized

$$\mathcal{L}_{TB-recon} = \mathcal{L}_{recon} + \alpha \cdot \mathcal{L}_{segm}$$

$$\mathcal{L}_{recon} = 1 - SSIM(\hat{y}_{recon}, y_{recon}) + \beta \cdot MAE(\hat{y}_{recon}, y_{recon})$$

$$\mathcal{L}_{segm} = 1 - DICE(\hat{y}_{segm}, y_{segm}) + \gamma \cdot NLL(\hat{y}_{segm}, y_{segm})$$

with α , β and γ empirically set to 1, 6.67^[2] and 0.01 respectively

- Monitored metric: Dice Similarity Coefficient (DSC)

^[1] Milletari, F., et al."V-net: Fully convolutional neural networks for volumetric medical image segmentation." Fourth International Conference on 3DV. IEEE, 2016.

^[2] Zhao, H., Gallo, O., Frosio, I., & Kautz, J. (2016). Loss functions for image restoration with neural networks. *IEEE Transactions on computational imaging*, 3(1), 47-57.

Network trained end-to-end

- The network is trained for 500k iterations
- 20 epochs early-stopping
- 5% dropout rate^[3]
- Adam optimizer^[4] (learning rate = 1E-5)
- NVIDIA V100 32GB GPU
- Python 3.6.5 and Tensorflow 1.12

^[3] Srivastava, N., Hinton, G., Krizhevsky, A., Sutskever, I., & Salakhutdinov, R. (2014). Dropout: a simple way to prevent neural networks from overfitting. *The journal of machine learning research*, 15(1), 1929-1958.

^[4] Kingma, D. P., & Ba, J. (2014). Adam: A method for stochastic optimization. *arXiv preprint arXiv:1412.6980*.

Imaging data

- 174 knees from 87 participants to the Osteoarthritis Initiative study (OAI)^[5]
- 3D sagittal double-echo steady-state (DESS) MRI scans
- Acquisition parameters:
 - 3.0T Siemens Trio at two time points.
 - TR 16.2ms
 - TE 4.7ms
 - FOV 14cm
 - Readout bandwidth 185kHz
 - Matrix size 384x384x160
 - Resolution 0.364x0.364x0.7mm

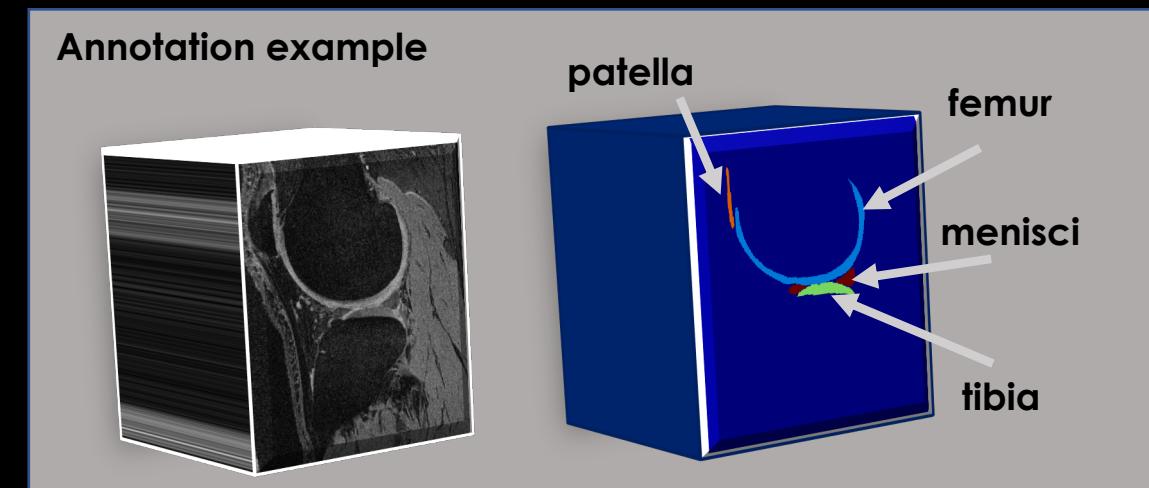


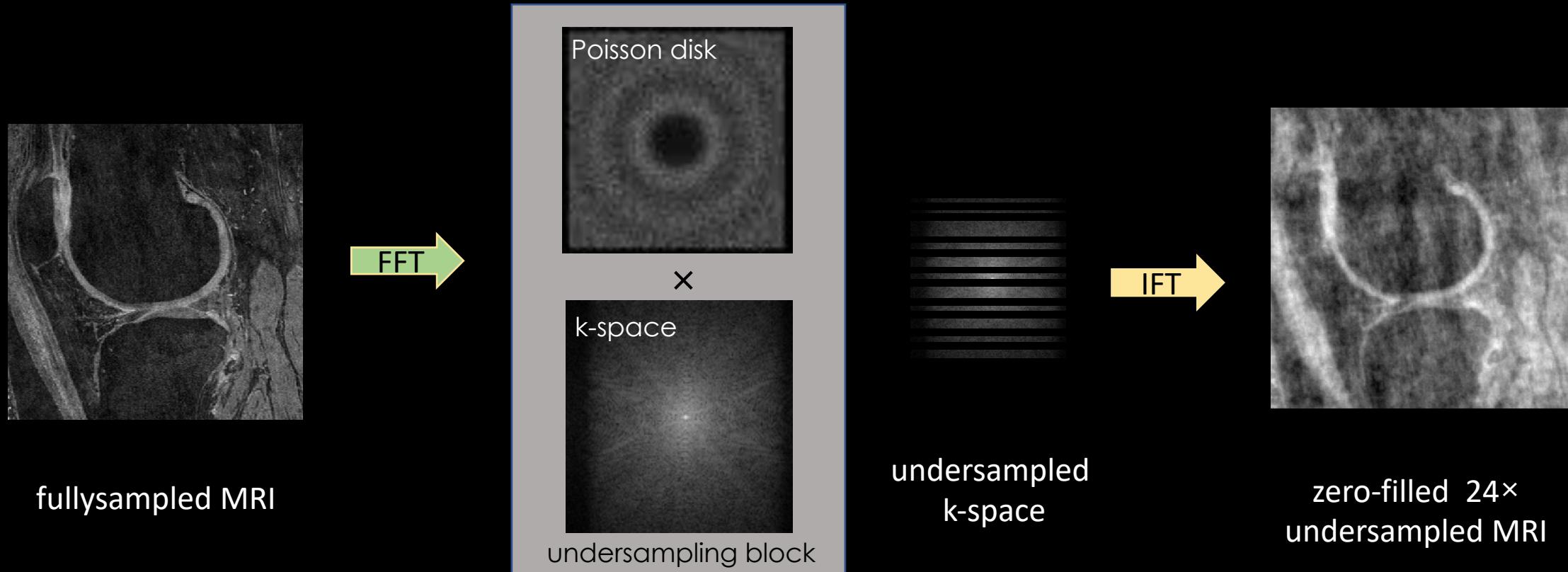
Table 1 Population attributes distribution in training validation and test splits. Race is reported in non-White/White or Caucasian/Black or African American/Asian order; sex in male/female order.

	Training	Validation	Test
Age	59.37±9.09	58.57±9.51	70.86±7.40
BMI [kg/m ²]	30.49±4.21	33.30±6.01	31.23±3.90
Race	1/47/11/0	0/8/6/0	1/13/0/0
Sex	28/31	8/6	9/5

^[5] Peterfy, C. G., Schneider, E., & Nevitt, M. (2008). The osteoarthritis initiative: report on the design rationale for the magnetic resonance imaging protocol for the knee. *Osteoarthritis and cartilage*, 16(12), 1433-1441.

Retrospective undersampling

- Variable-density Poisson disk undersampling mask^[6]
- 5 acceleration factors (AF) 2x, 4x, 6x, 12x, 24x
- Retrospective undersampling performed using the SigPy software^[7]

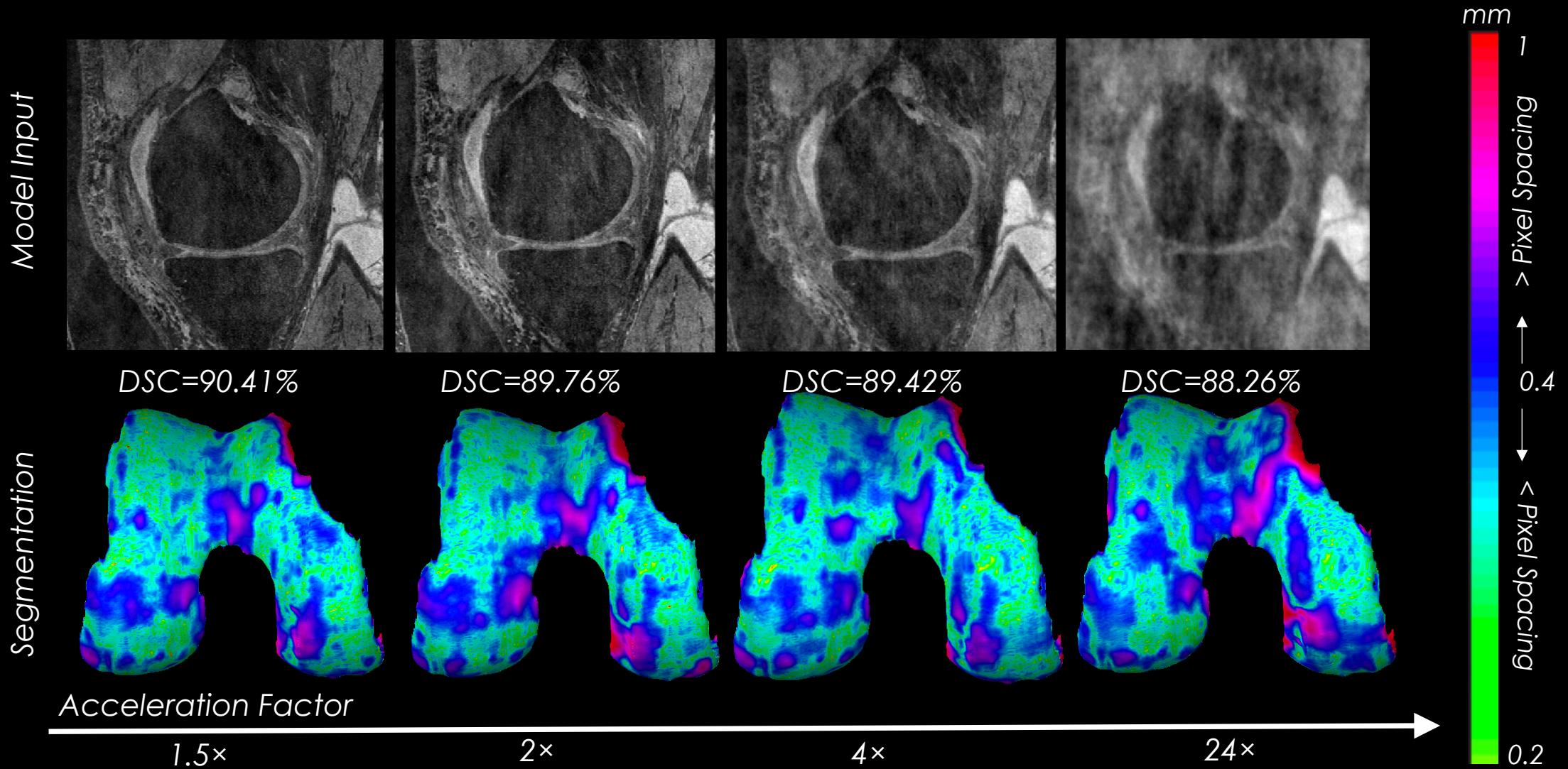


^[6] Bridson, R.. “Fast Poisson disk sampling in arbitrary dimensions.” SIGGRAPH sketches. 2007.

^[7] <http://indexsmart.mirasmart.com/ISMRM2019/PDFfiles/4819.html>

Results – TB-recon's femural cartilage segmentation

Point by Point distance between automatic and manual segmentation



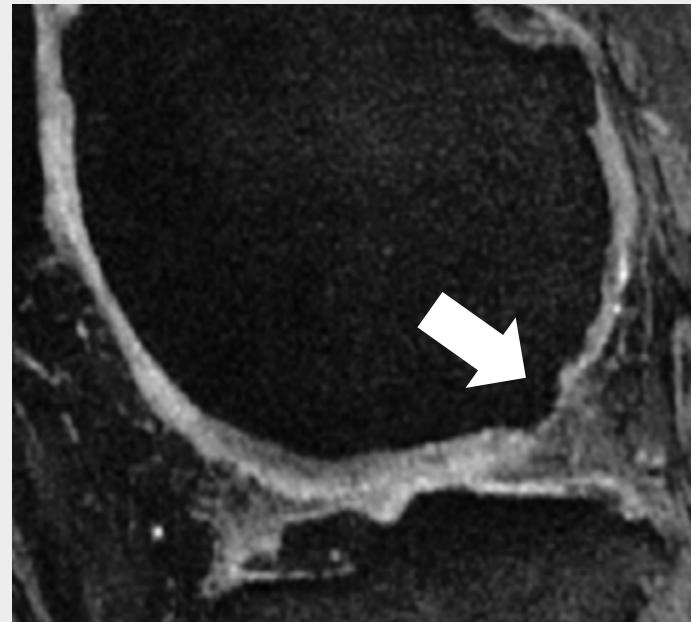
Results – TB-recon Reconstruction

Bone marrow edema visible in a sagittal DESS (A), is well observed at 6 \times (B) and 12 \times (B) AFs reconstructed MRIs

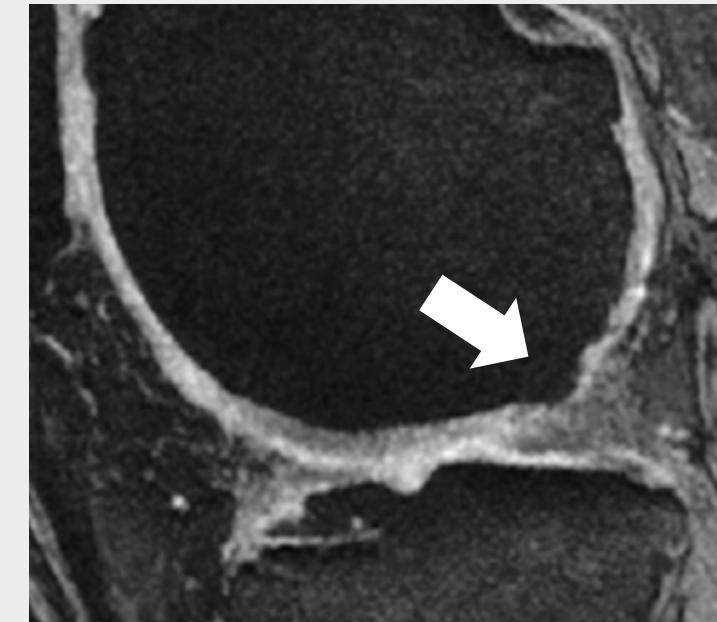
DESS



AF=6 \times



AF=12 \times



Results – Ablation study

Investigated importance of:

- MRI reconstruction
- Inter-task skip connections

Femur - DSC	4×	6×	24×
<i>TB-recon</i>	87.33±1.93	87.58±1.79	85.63±2.56

Tibia - DSC	4×	6×	24×
<i>TB-recon</i>	85.12±3.85	86.18±3.59	85.84±3.51

Patella - DSC	4×	6×	24×
<i>TB-recon</i>	82.10±6.83	81.76±7.82	77.65±7.96

Menisci - DSC	4×	6×	24×
<i>TB-recon</i>	84.91±2.79	83.78±3.06	82.28±2.64

Results – Ablation study

No MRI reconstruction

Femur - DSC	4×	6×	24×
<i>TB-recon</i>	87.33±1.93	87.58±1.79	85.63±2.56
<i>zero-filled</i>	82.27±2.75	81.79±2.73	16.27±0.91
Tibia - DSC	4×	6×	24×
<i>TB-recon</i>	85.12±3.85	86.18±3.59	85.84±3.51
<i>zero-filled</i>	83.32±4.53	81.26±5.20	29.75±1.80
Patella - DSC	4×	6×	24×
<i>TB-recon</i>	82.10±6.83	81.76±7.82	77.65±7.96
<i>zero-filled</i>	78.10±7.17	77.37±6.47	70.88±10.59
Menisci - DSC	4×	6×	24×
<i>TB-recon</i>	84.91±2.79	83.78±3.06	82.28±2.64
<i>zero-filled</i>	81.87±2.99	81.61±3.15	16.69±0.93

bold = significant
outperformance

Results – Ablation study

Femur - DSC	4×	6×	24×
<i>TB-recon</i>	87.33±1.93	87.58±1.79	85.63±2.56
<i>zero-filled</i>	82.27±2.75	81.79±2.73	16.27±0.91
<i>naïve</i>	84.97±2.69	82.94±2.99	83.71±2.82
Tibia - DSC	4×	6×	24×
<i>TB-recon</i>	85.12±3.85	86.18±3.59	85.84±3.51
<i>zero-filled</i>	83.32±4.53	81.26±5.20	29.75±1.80
<i>naïve</i>	84.09±3.86	83.26±4.20	56.15±2.38
Patella - DSC	4×	6×	24×
<i>TB-recon</i>	82.10±6.83	81.76±7.82	77.65±7.96
<i>zero-filled</i>	78.10±7.17	77.37±6.47	70.88±10.59
<i>naïve</i>	53.74±4.36	77.62±7.61	32.45±2.24
Menisci - DSC	4×	6×	24×
<i>TB-recon</i>	84.91±2.79	83.78±3.06	82.28±2.64
<i>zero-filled</i>	81.87±2.99	81.61±3.15	16.69±0.93
<i>naïve</i>	82.35±2.69	81.47±3.31	54.59±2.24

No MRI reconstruction

No inter-task skip connections

bold = significant outperformance

No MRI recon

task skip
ctions

For more details on our work, including additional experiments
please refer to our paper #239

Caliva, F. Leynes, A., Shah, R., Bharadwaj, U. U., Majumdar, S., Larson, P., & Pedoia, V. (2020, January). Breaking Speed Limits with Simultaneous Ultra-Fast MRI Reconstruction and Tissue Segmentation. In Medical Imaging with Deep Learning

	4×	6×	24×
Femur - DSC			
<i>TB-recon</i>	87.33±1.93	87.58±1.79	85.63±2.56
<i>zero-filled</i>	82.27±2.75	81.79±2.73	16.27±0.91
<i>naïve</i>	82.35±2.69	81.47±3.31	54.59±2.24

bold = significant
outperformance

Contributions

- **TB-recon** for task-based MRI reconstruction
- Segmentation at **ultra-high acceleration factors** is possible
- The proposed **shared encoder + inter-task** skip connections facilitate segmentation

Broader impact

Task-based reconstruction can break speed limits, which have hampered the application of magnetic resonance imaging

Potential applications:

- disease and abnormality identification
- organ volume estimation
- lesion size and counting (e.g. multiple sclerosis and micro-bleeds)

**We hope this paper further stimulates
research community's interest on task-based fast MRI**

Acknowledgements

Valentina Pedoia's Lab

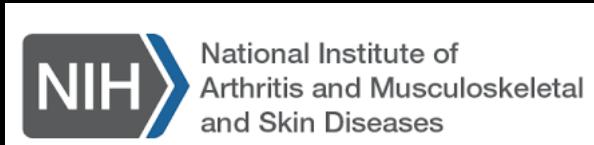
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Adam Noworolski

Sharmila Majumdar's Lab

Upasana Upadhyay Bharadwaj
Claudia Iriondo

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