



MRC Cognition
and Brain
Sciences Unit



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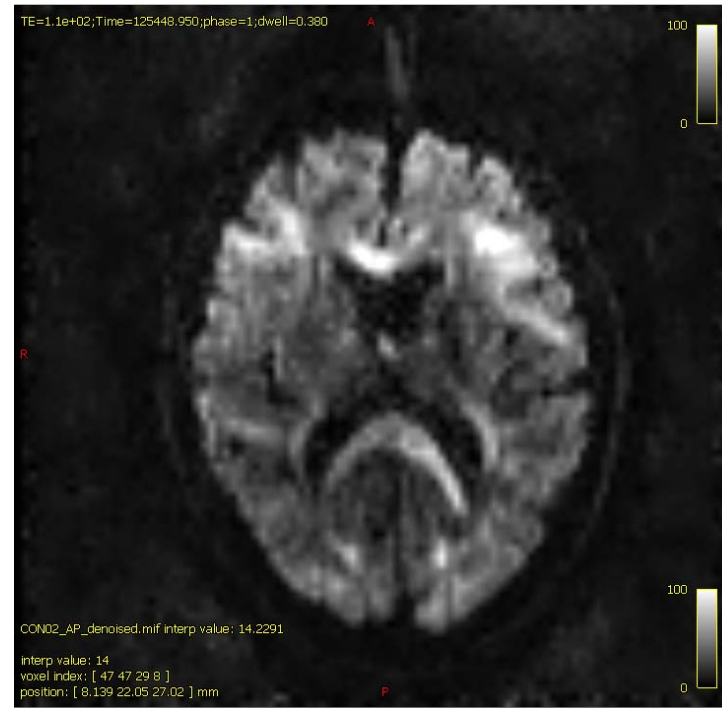
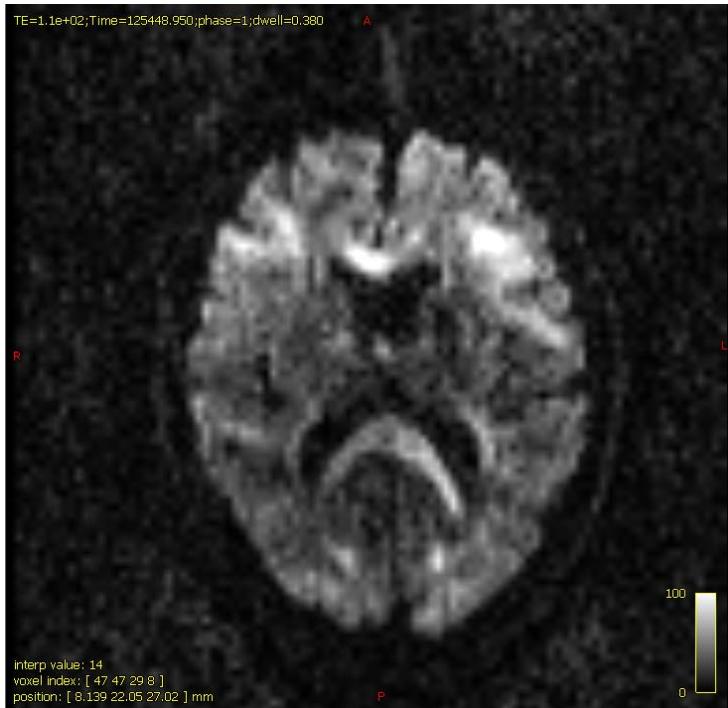
Diffusion MRI: preprocessing, model fitting and TBSS

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MRC Cognition and Brain Sciences Unit

Preprocessing

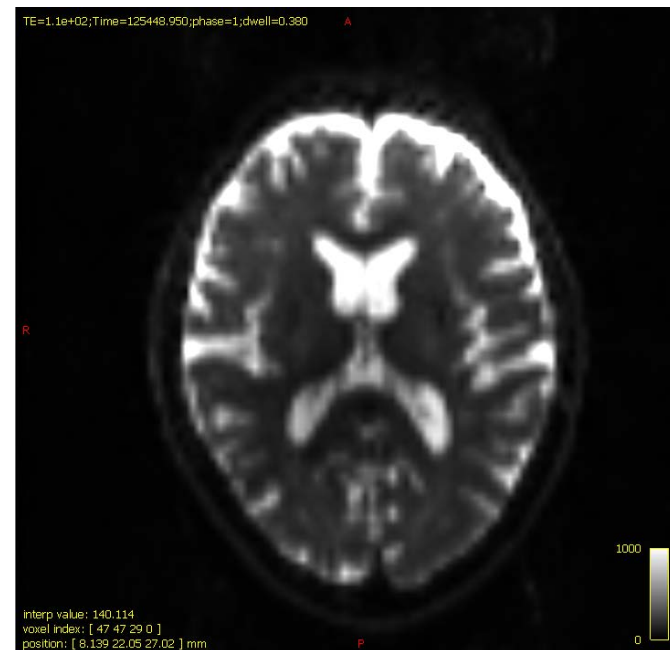
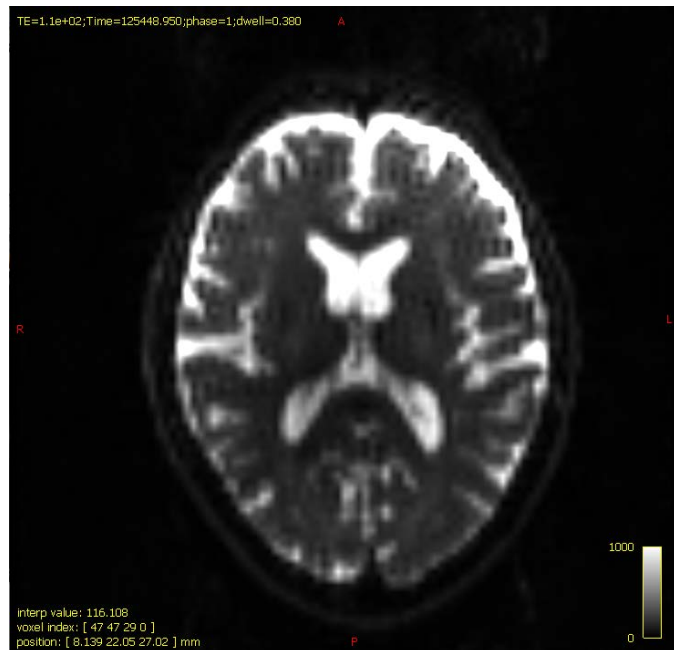
DWI denoising

- Denoising must be performed as the first step of the pipeline
- Exploits data redundancy in the patch-level PCA domain



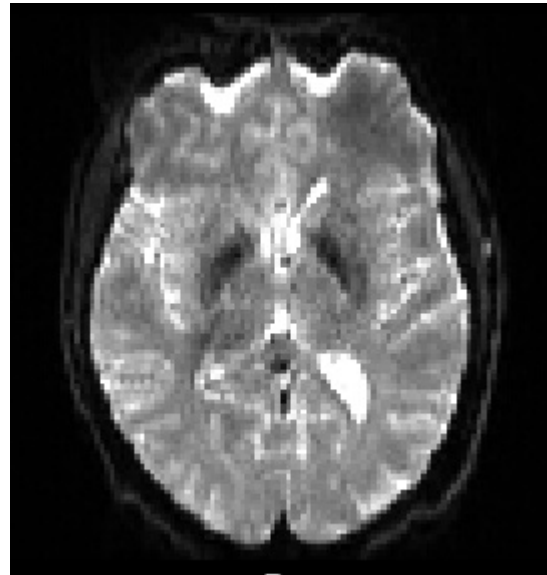
Removal of Gibbs artefacts (optional)

- Removes Gibbs ringing artefacts from DWI images
- Designed for data acquired with full k-space
- May fail for data acquired with Partial Fourier – always inspect the output

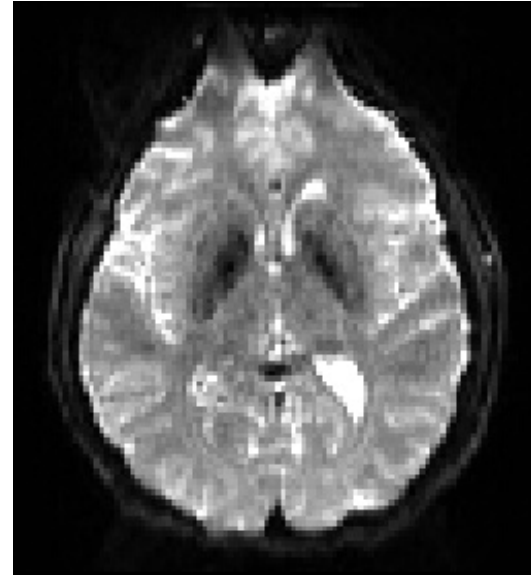


TOPUP: correction for EPI distortions

- EPI distortion due to B0 inhomogeneity depends on phase-encode direction



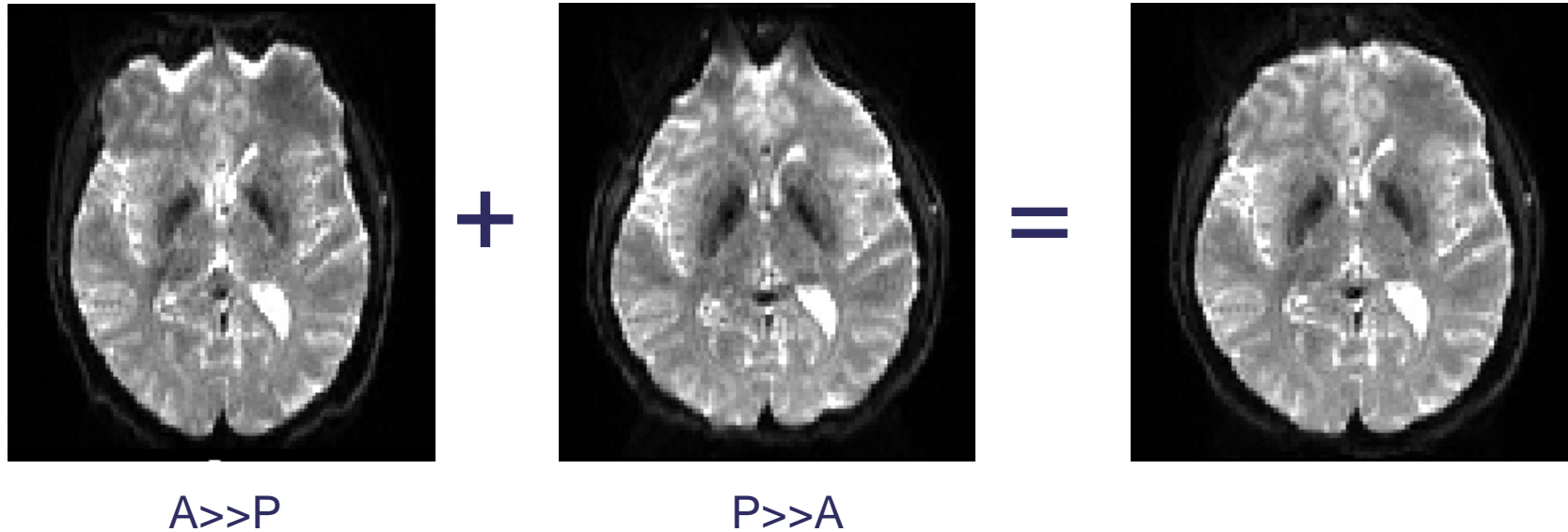
A>>P



P>>A

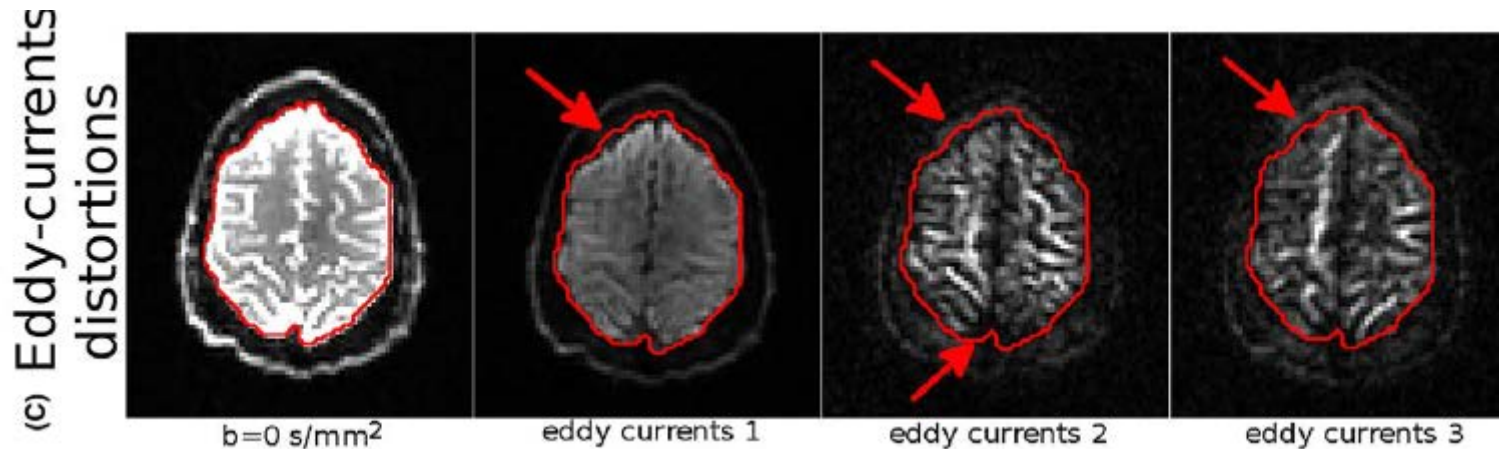
TOPUP: correction for EPI distortions

- EPI distortion due to B0 inhomogeneity depends on phase-encode direction
- Can it be corrected?



EDDY: correction for eddy currents and motion

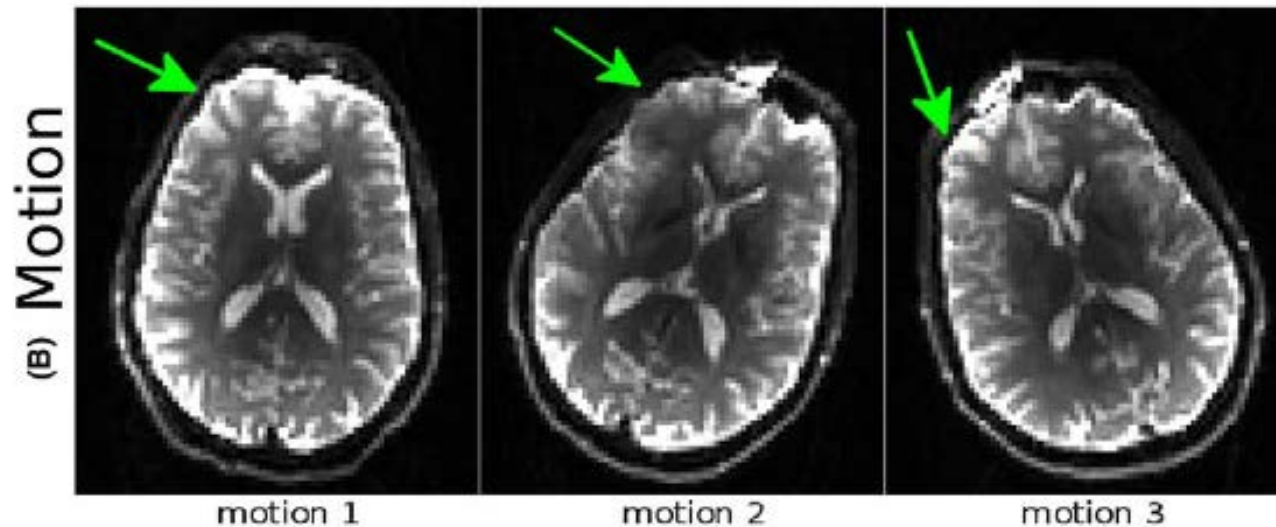
- Eddy-current distortions occur due to the rapid switching of diffusion gradients.
- Depend on gradient magnitude and direction.
- They affect the diffusion weighted images (DWI) but not the $b=0$ image.
- Results in mismatching between $b=0$ and DWI volumes.



Irfanoglu et al, MRM 2018

EDDY: correction for eddy currents and motion

- Motion artefacts occur due to involuntary head movements.
- Results in mismatching between DWI volumes.
- Can also result in signal changes due to coil sensitivity.



Irfanoglu et al, MRM 2018

EDDY QC: quality control

- For individual subjects: eddy_quad

Volume-to-volume motion

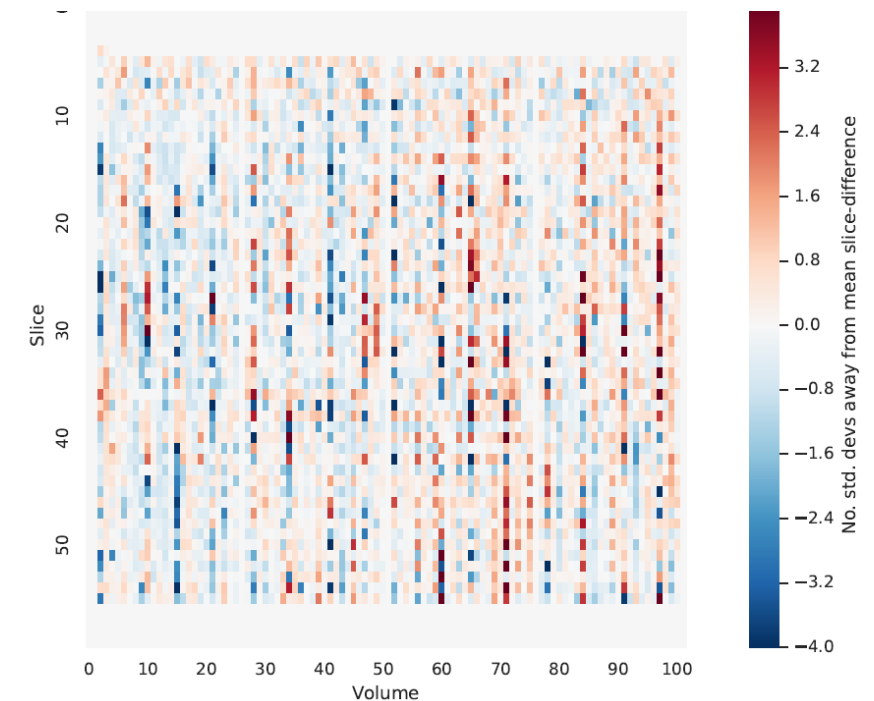
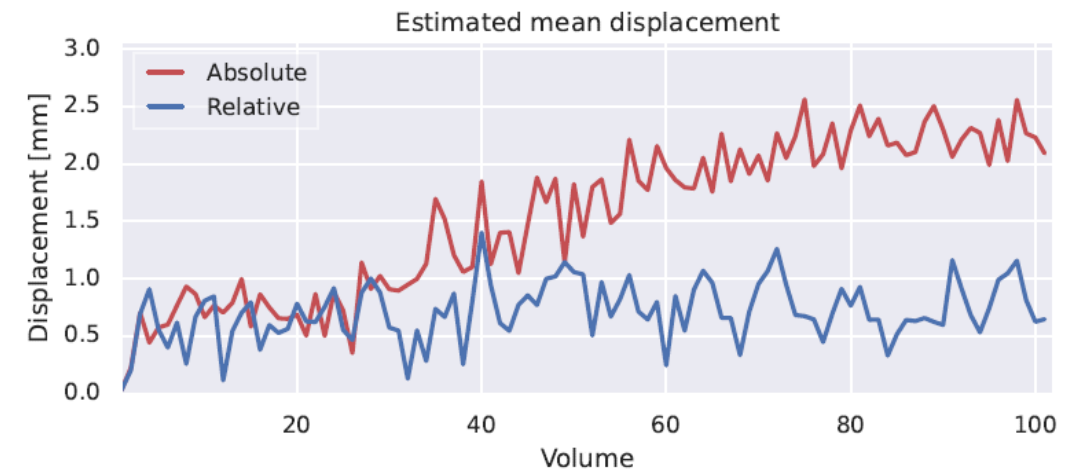
Average abs. motion (mm)	1.52
Average rel. motion (mm)	0.70
Average x translation (mm)	0.10
Average y translation (mm)	-0.90
Average z translation (mm)	0.98
Average x rotation (deg)	-0.02
Average y rotation (deg)	0.19
Average z rotation (deg)	-0.15

Outliers

Total outliers (%)	0.45
Outliers (b=700 s/mm ²)	2.71
Outliers (b=1200 s/mm ²)	0.00
Outliers (b=2800 s/mm ²)	0.00
Outliers (PE dir=[0. 1. 0.])	0.42

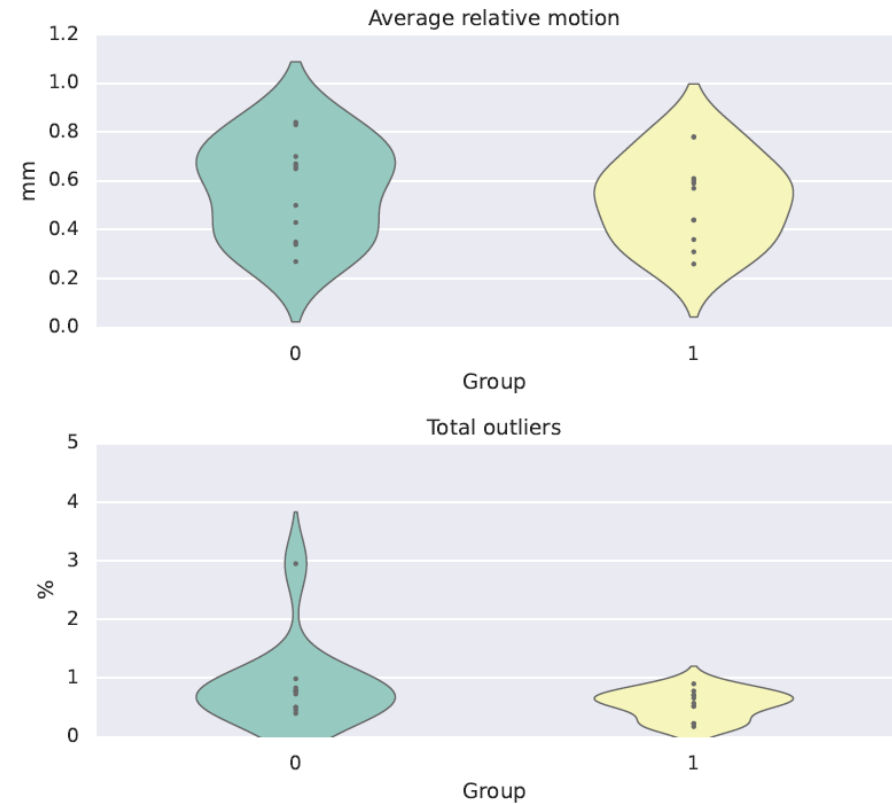
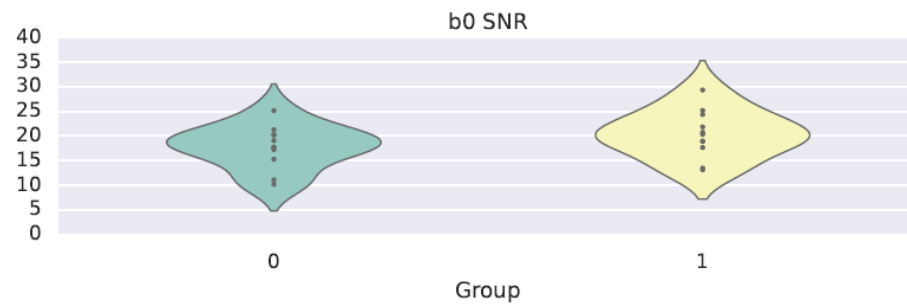
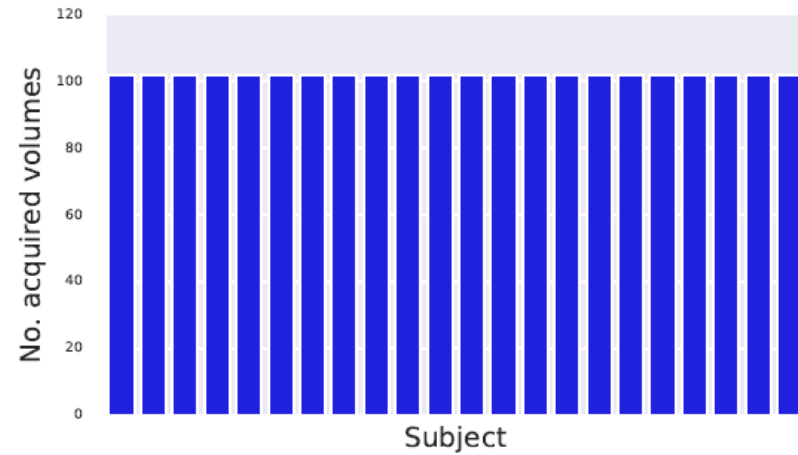
SNR/CNR

Average SNR (b=0 s/mm ²)	17.57
Average CNR (b=700 s/mm ²)	0.96
Average CNR (b=1200 s/mm ²)	1.33
Average CNR (b=2800 s/mm ²)	1.54



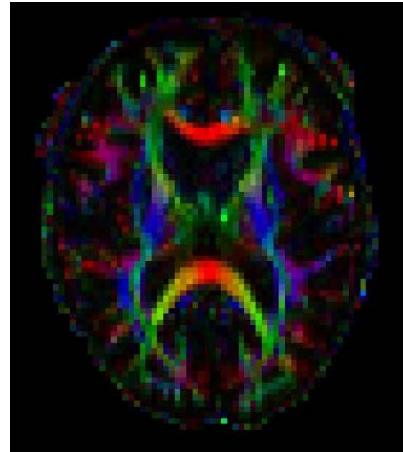
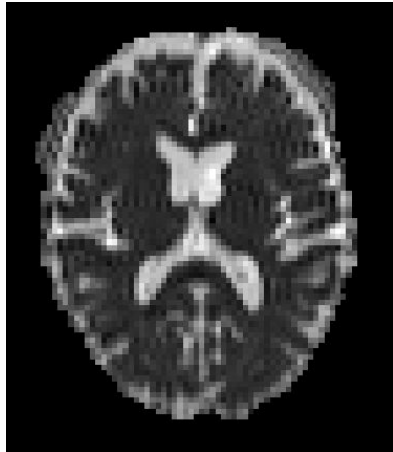
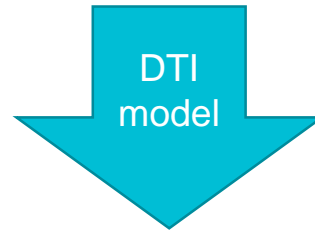
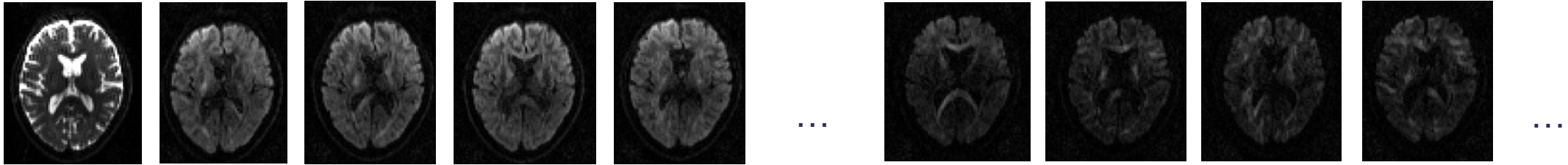
EDDY QC: quality control

- Study-wise quality control: eddy_squad

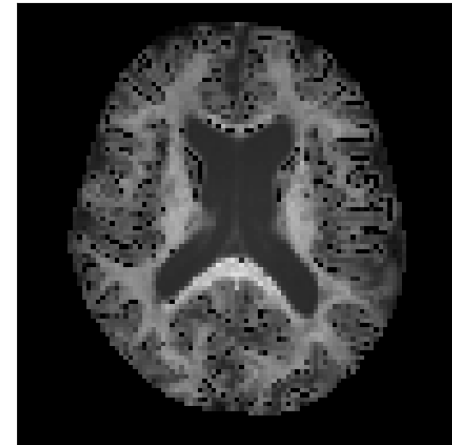
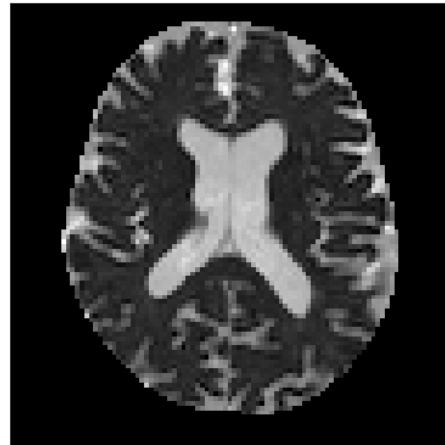
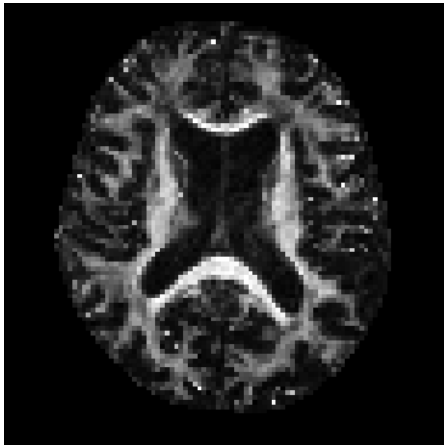
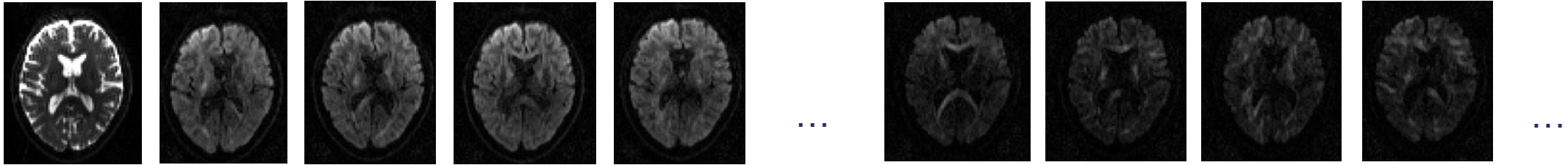


Model fitting

DTI: diffusion tensor model fitting



DKI: diffusion kurtosis model fitting

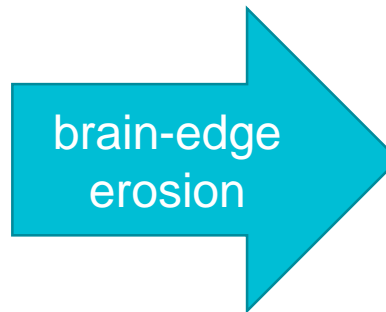
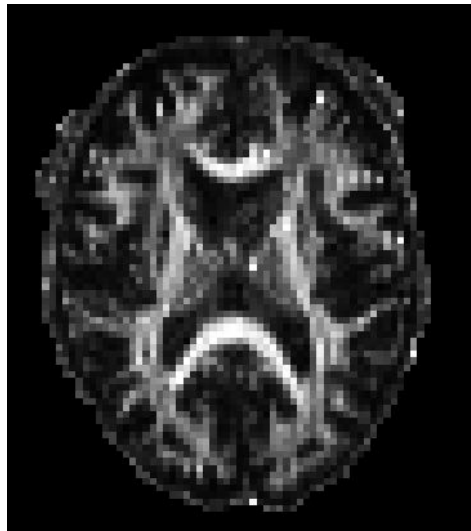


Group Analysis: TBSS

TBSS: Group Analysis of DTI data

1. Preparing FA data for TBSS:

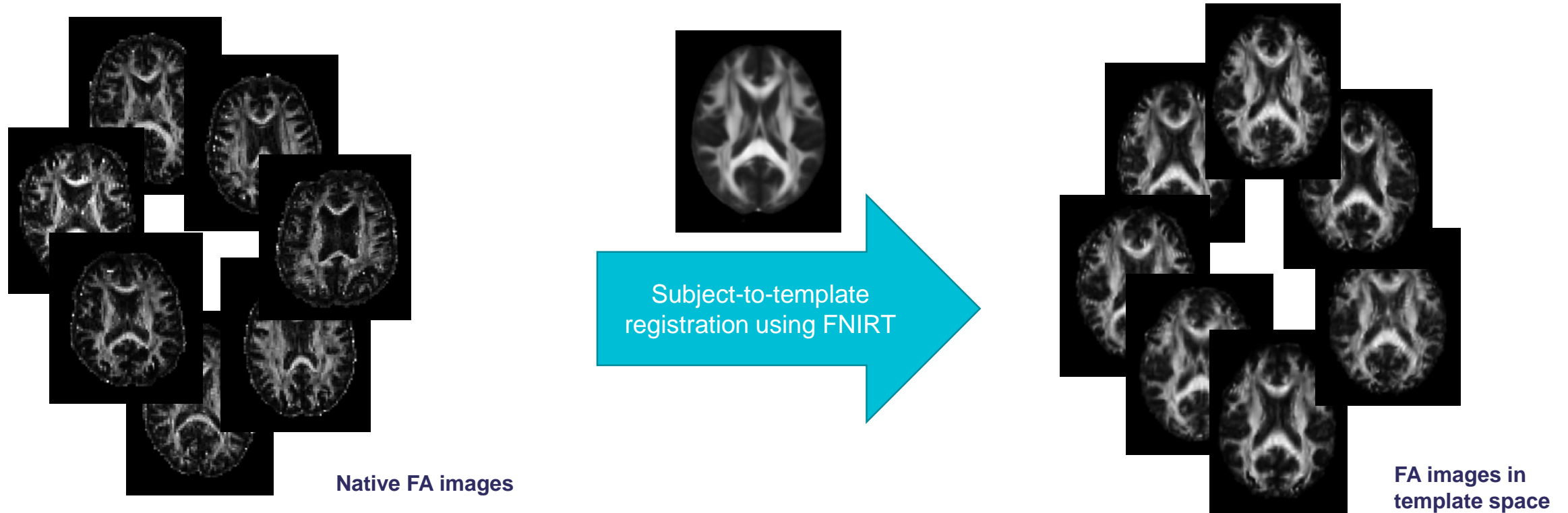
- Rename files
- New folder structure
- Erode FA images to reduce brain-edge artefacts



TBSS: Group Analysis of DTI data

2. Registering the FA data:

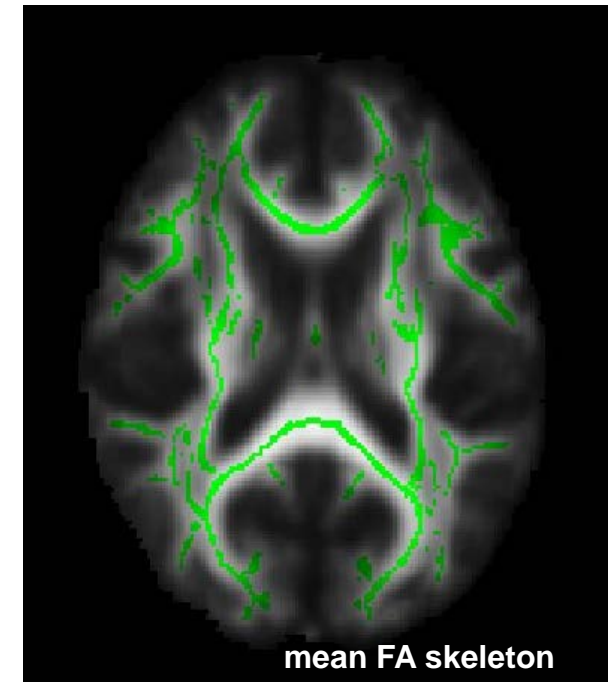
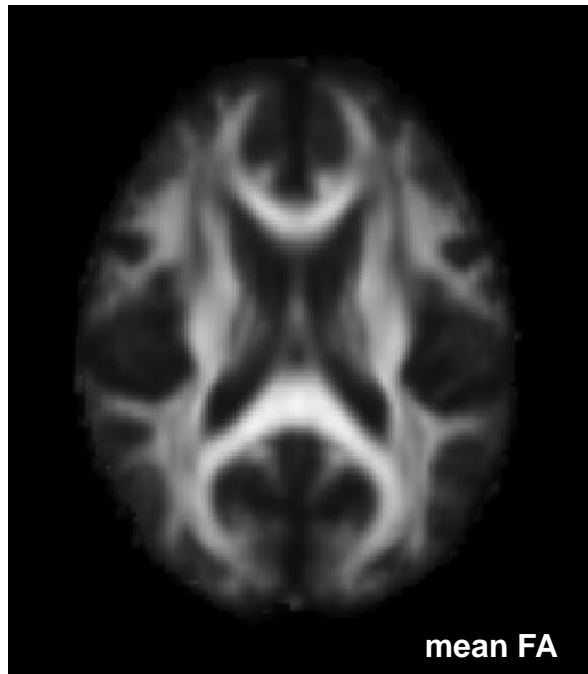
- Register FA images to the FMRIB58_FA template using non-linear registration (FNIRT)



TBSS: Group Analysis of DTI data

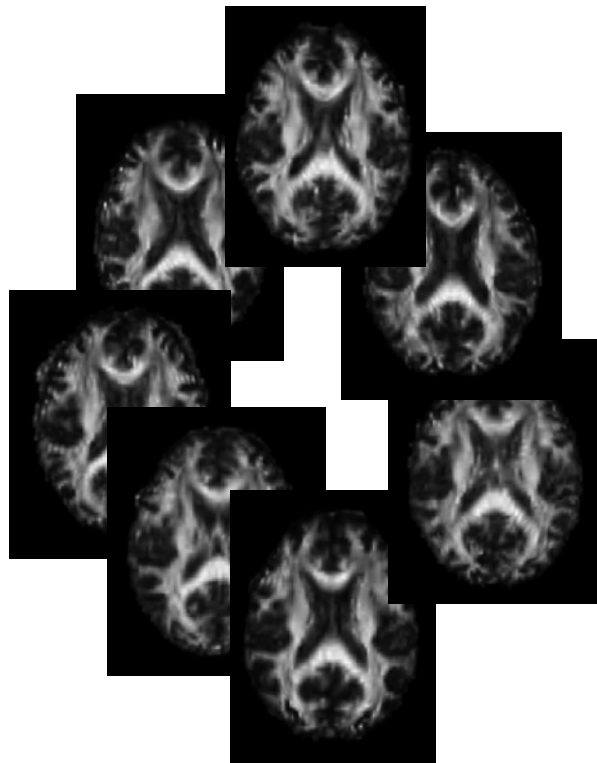
3. Post-registration processing:

- Average all registered FA images
- Create the mean FA skeleton

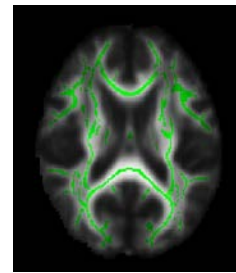


TBSS: Group Analysis of DTI data

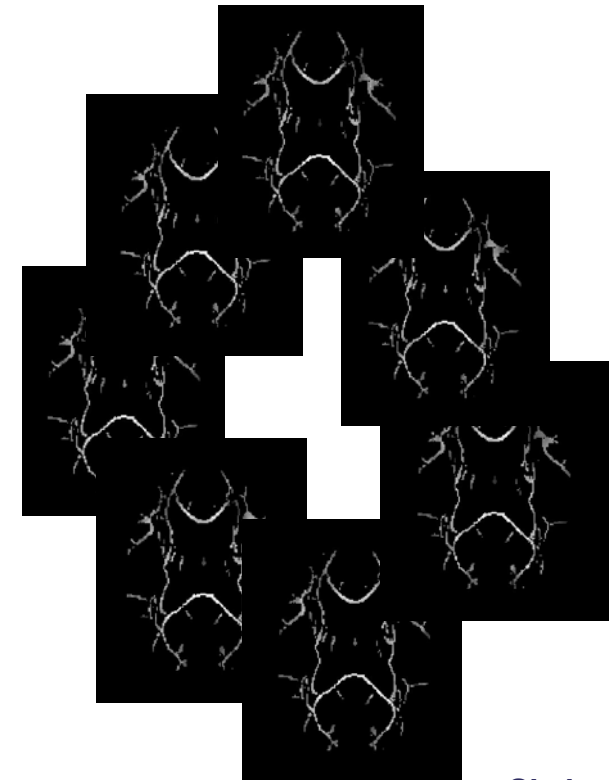
4. Projecting each subject's FA map onto the skeleton:



FA images in
template space



Projection onto
skeleton

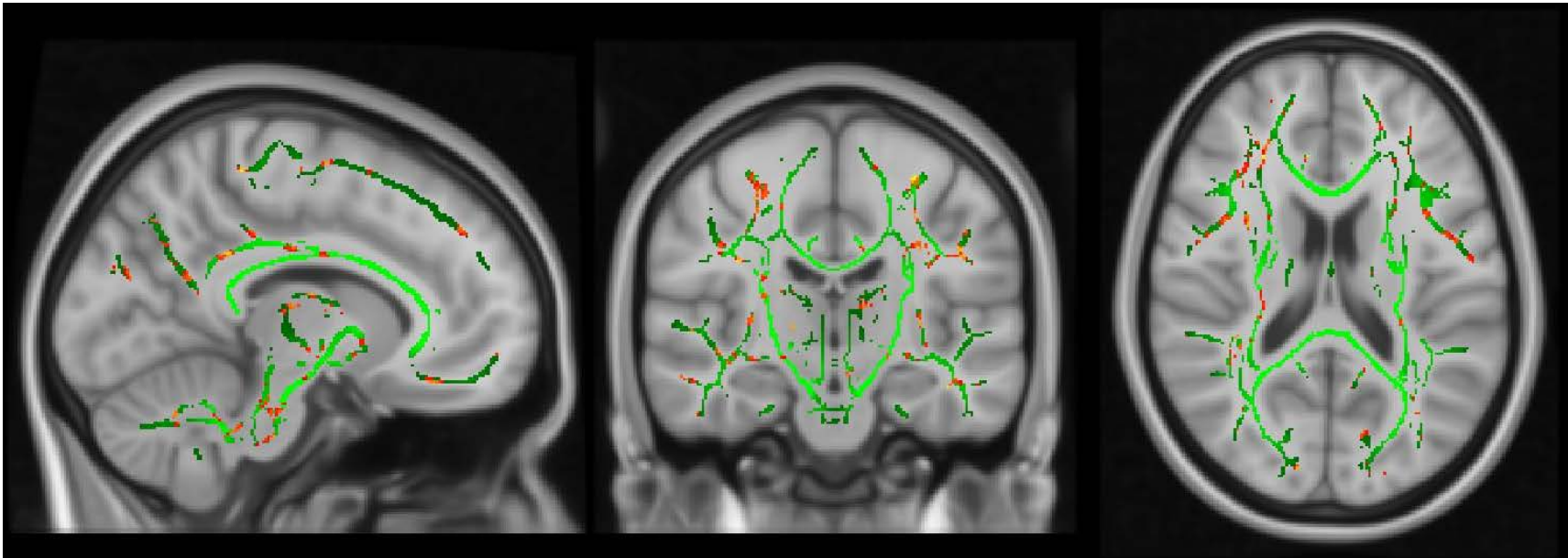


Skeletonised FA
images

VBM using FSL tools

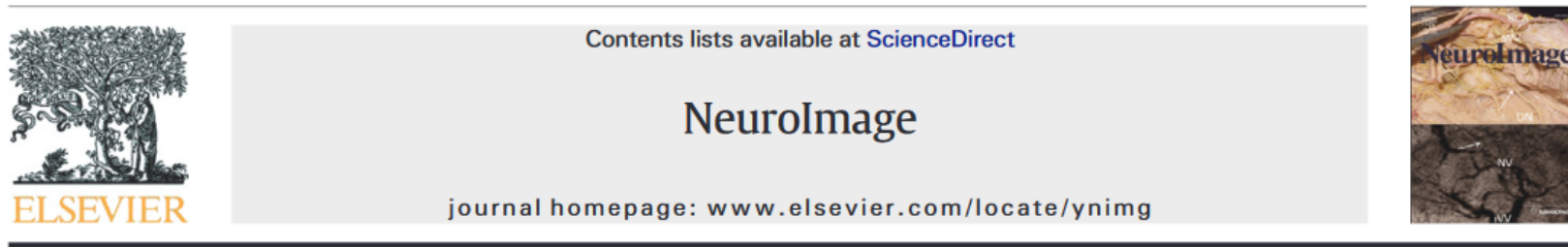
5. Statistical analysis:

- Create the design matrix
- Use **randomise** for non-parametric inference



Interpretation of results

- FA skeleton does not represent the center of a specific WM tract.
- Significance maps should be interpreted with care: post-registration misalignments and voxel misassignments may confound the FA values from structures in close proximity.
- Choice of parameters, e.g. the registration target, can lead to large variation in the FA skeleton and subsequently the statistical results.



Methodological considerations on tract-based spatial statistics (TBSS)

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Bram Stieltjes ^a, Klaus H. Maier-Hein ^{a,e,*}





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Questions?