



MRC Cognition  
and Brain  
Sciences Unit



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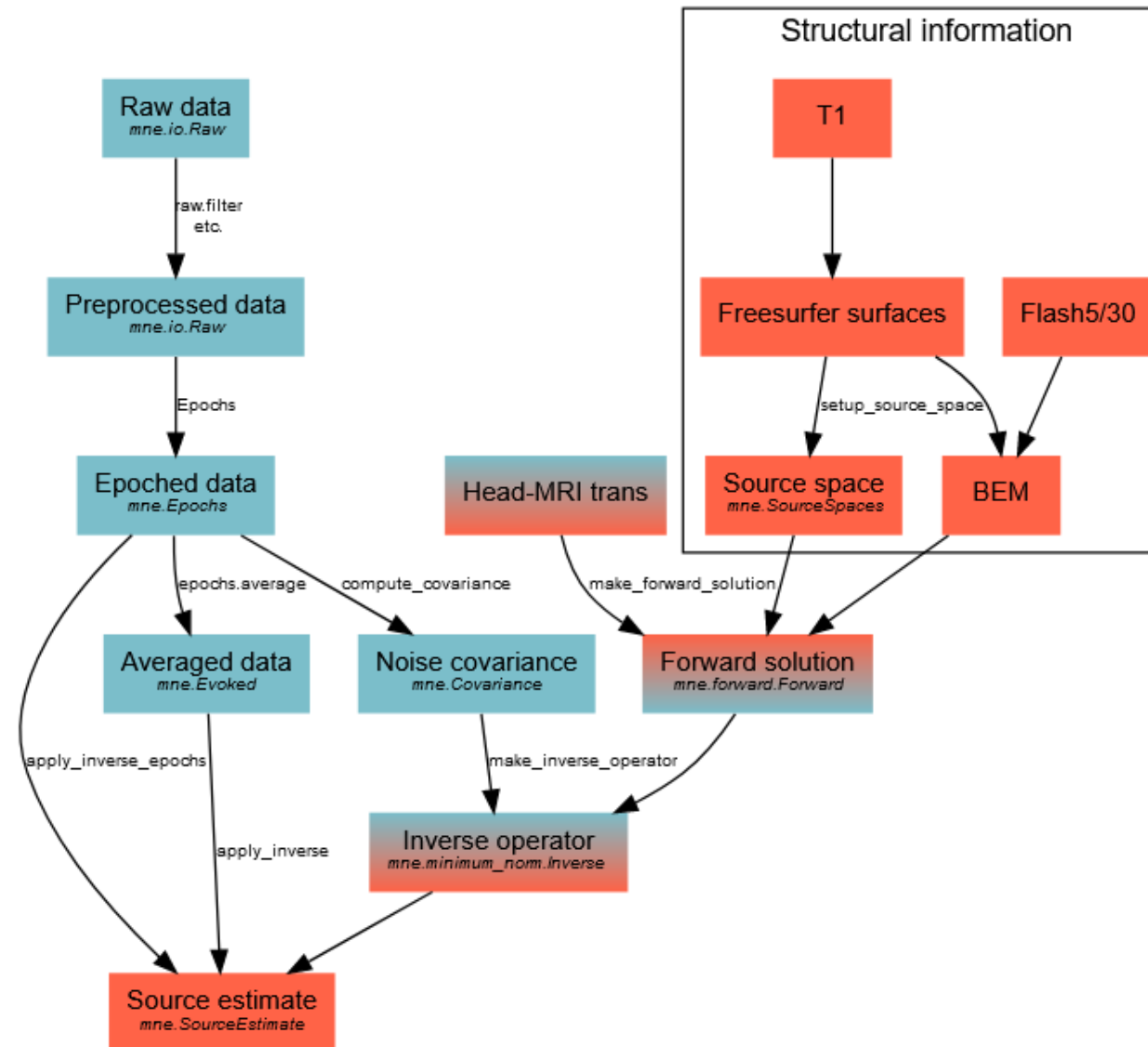
# EEG/MEG 1:

**Pre-processing – spectral and spatial filtering**

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# Typical EEG/MEG Analysis Pipeline



# Data Pre-Processing - Artefacts

What are the artefacts of data pre-processing?

# Artefacts

- **non-physiological**, i.e. from outside the body (sensor-intrinsic noise, line noise, moving objects, vibrations)  
=> Maxfilter (SSS), Frequency-Filtering, SSP, PCA/ICA
- **Physiological but non-brain**, e.g. eye movements, muscles  
=> SSP, PCA/ICA, H/L-Filtering
- **Physiological from the brain**, i.e. brain sources that are not of interest or not included in your source model  
=> choose appropriate source estimation, regularisation

## Wisdoms:

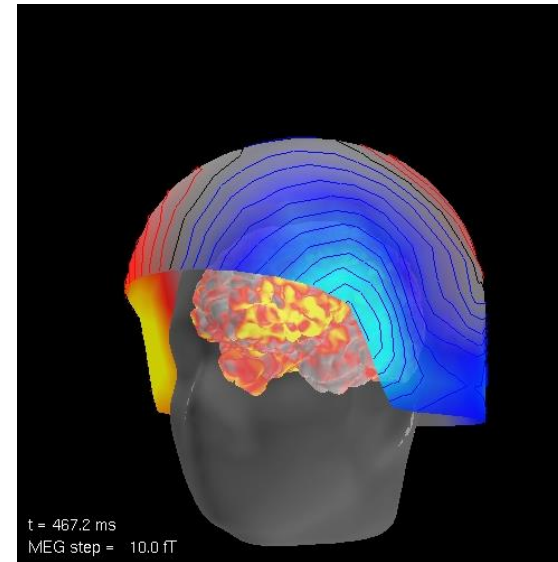
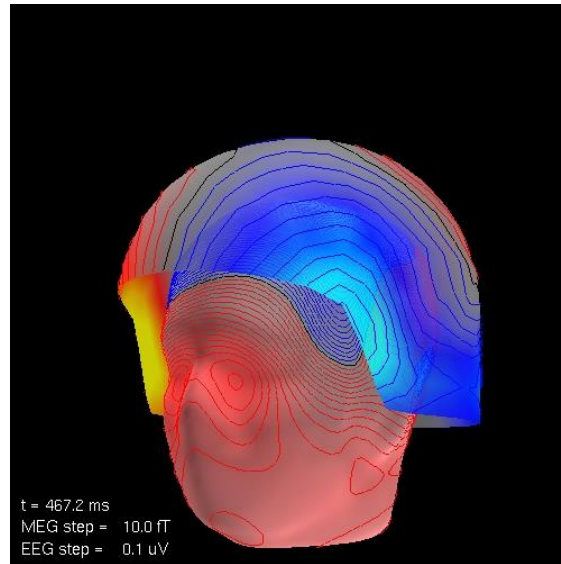
“Some people’s signal is other people’s noise.”

Unfortunately, you cannot just choose what’s signals and what’s noise.

It’s always better to avoid artefacts than to correct them.

# Artefacts in EEG and MEG Will End Up in Source Space

## Eye Blink



This will affect all source estimation methods —  
get rid of your artefacts beforehand.

# Separating Signal and Noise Components - “Decompositions”

You can decompose your signal in any way you want – the question is whether it can separate “interesting” from “non-so-interesting” parts of your data, either in space or time.

- 1) Define a set of “basis functions”, e.g.
  - a) A priori: sines/cosines, wavelets, polynomials.
  - b) Data driven: PCA/SVD/ICA, empirical modes.
- 2) Fit these basis functions to your data to explain (most of) its variance.
- 3) Select (or remove) those basis functions that you are (not) interested in, e.g. signal vs noise.
- 4) Reconstruct your signal with the components of interest.

If the basis functions are meaningful, you may be successful: cleaner data.

If the basis functions do not correspond to signal and noise parts of your data – you will get a result, but it will be distorted.

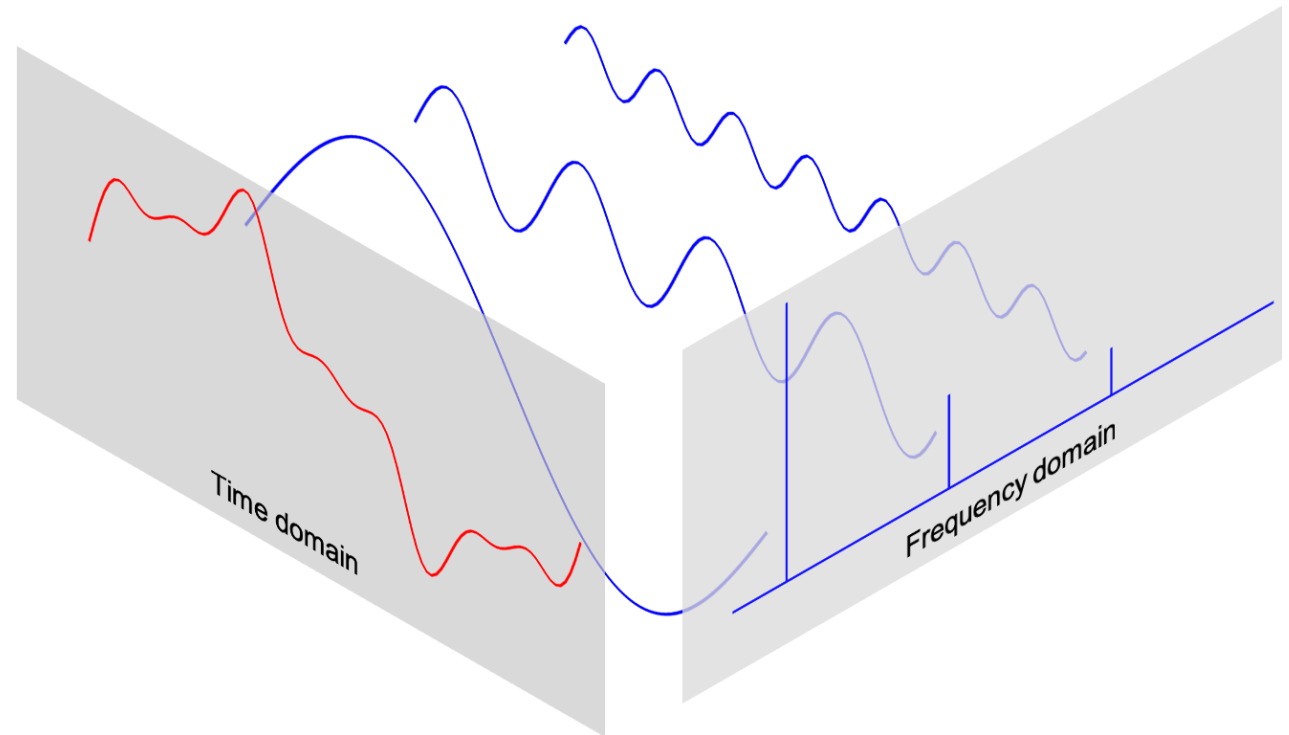
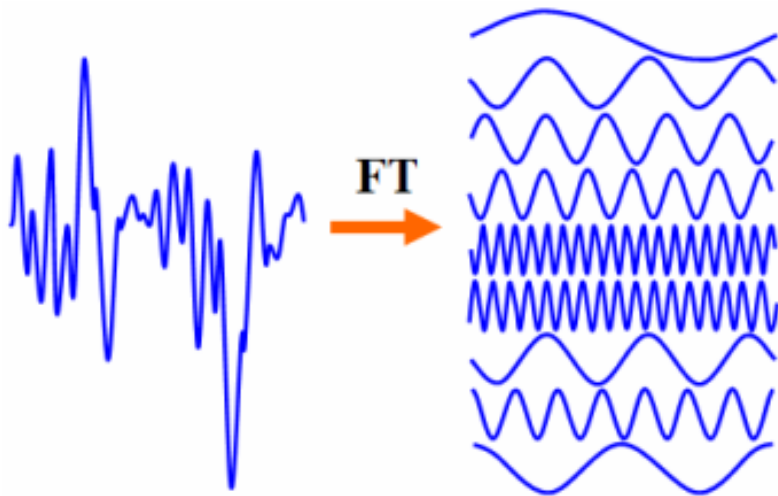
Think about what artefacts are the most relevant in your data, then decide which method is best to remove them:

1. How frequent?
2. How large? Time course and topography?
3. Are they related to your variables of interest?



# Time-Domain Signals Can Be Represented in the Frequency Domain - and Vice Versa

Decomposing signals  
into sine/cosine terms





# Basic Principals of Frequency Filtering

Filtering changes the time course of your data. Thus:

“Filter as much as necessary but as little as possible.”

Common types of filters:

“High-pass”: Lets higher frequencies pass, suppresses lower frequencies (incl. “detrending”)

“Low-pass”: Lets lower frequencies pass, removes higher frequencies

“Band-pass”: Lets frequencies within a frequency band pass, suppresses frequencies above and below the band

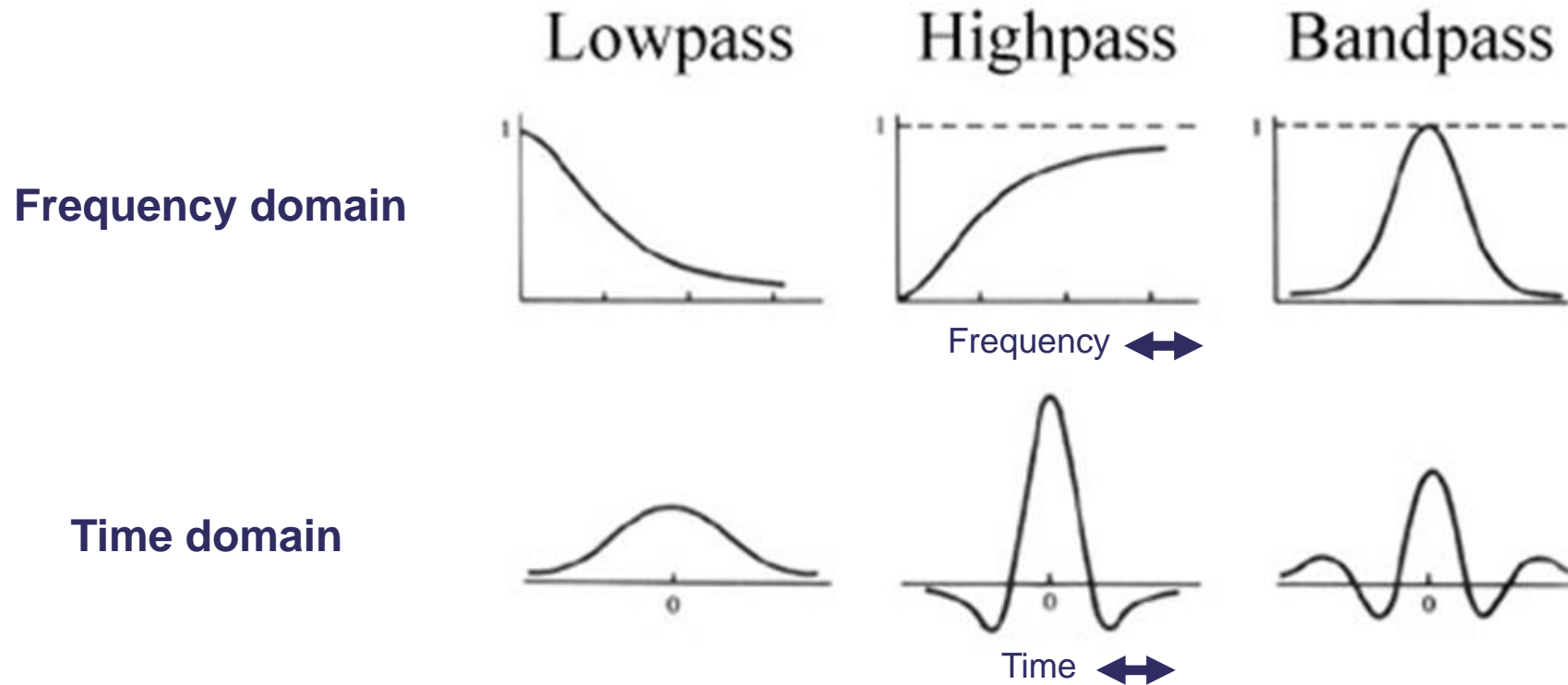
“Notch” filter: A very sharp band-pass filter, e.g. for 50 or 60 Hz line noise

(e.g. Cheveigen & Nelken, Neuron 2019, <https://www.sciencedirect.com/science/article/pii/S0896627319301746>), Widmann et al., Journal of Neuroscience Methods 2015, <https://www.sciencedirect.com/science/article/pii/S0165027014002866>, Tanner et al., Psychophysiology 2016, <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC4506207/>).

# Basic Principals of Frequency Filtering

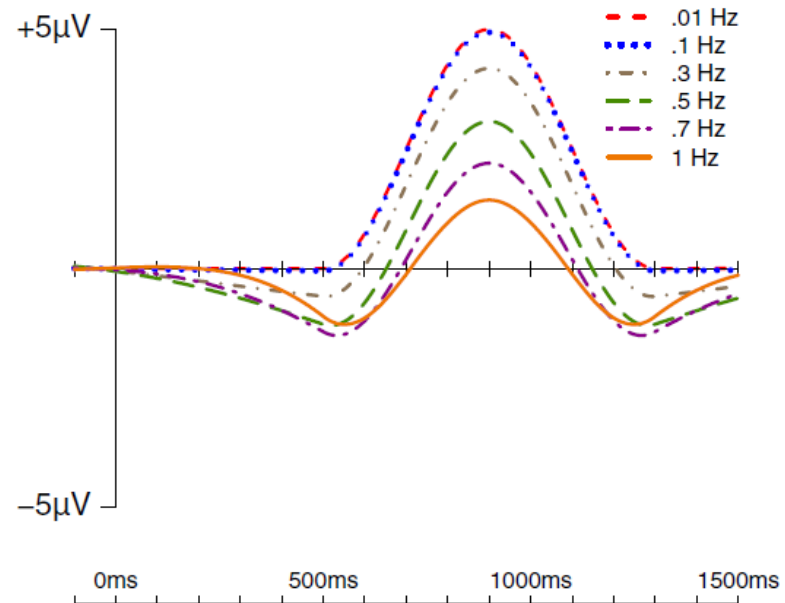
Time-domain and frequency-domain filtering are two sides of the same coin:

One type of frequency-domain filtering corresponds to one type of time-domain filtering.

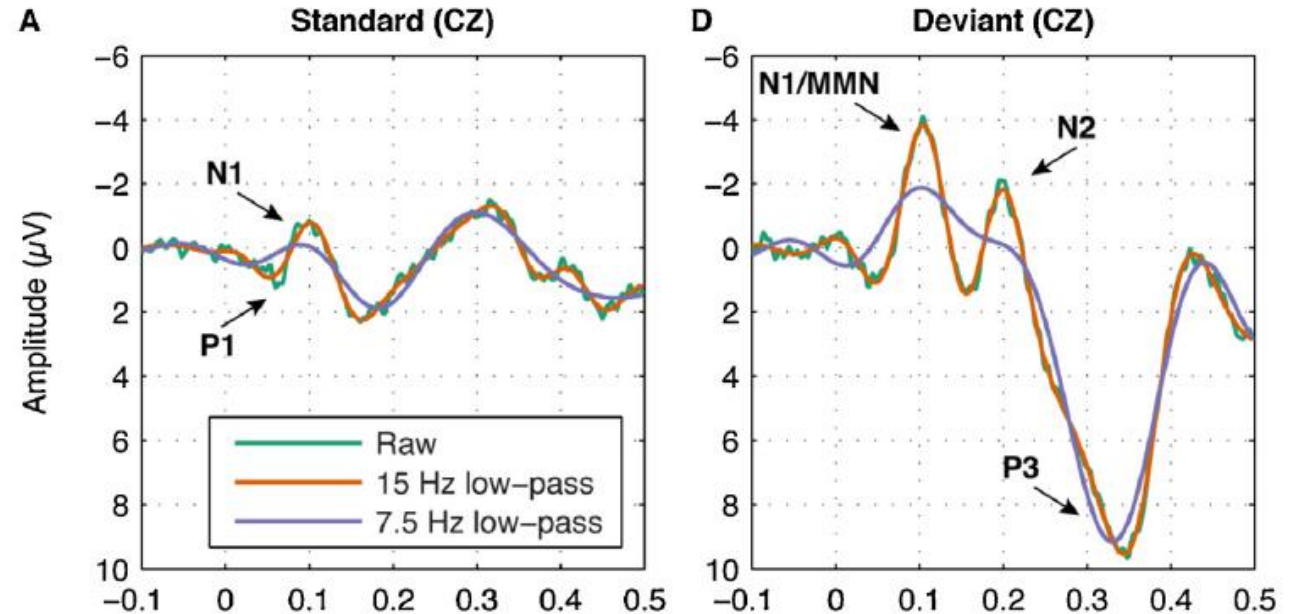


# Filtering can affect both signal and artefact

## High-pass filtering: “(linear/polynomial) Detrending” “Removing slow drifts”

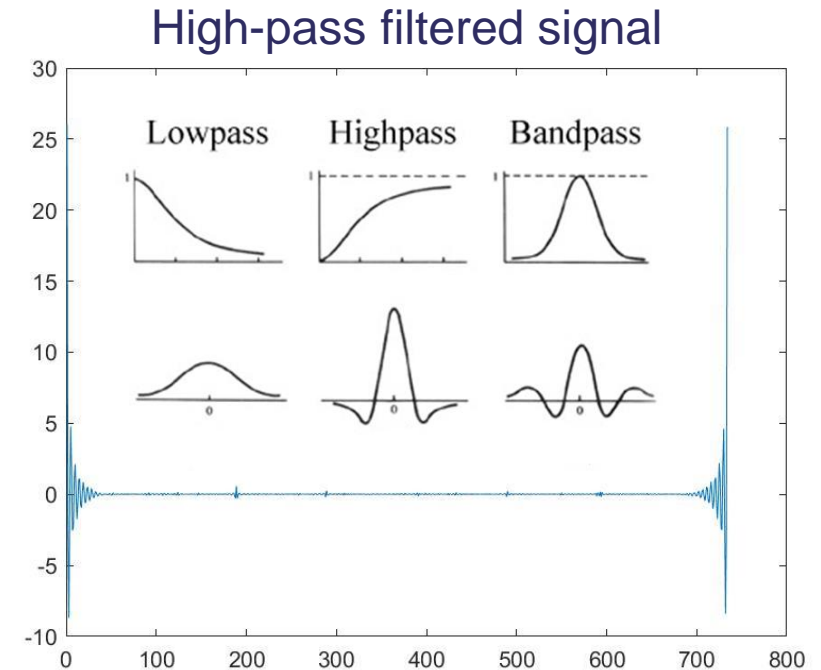
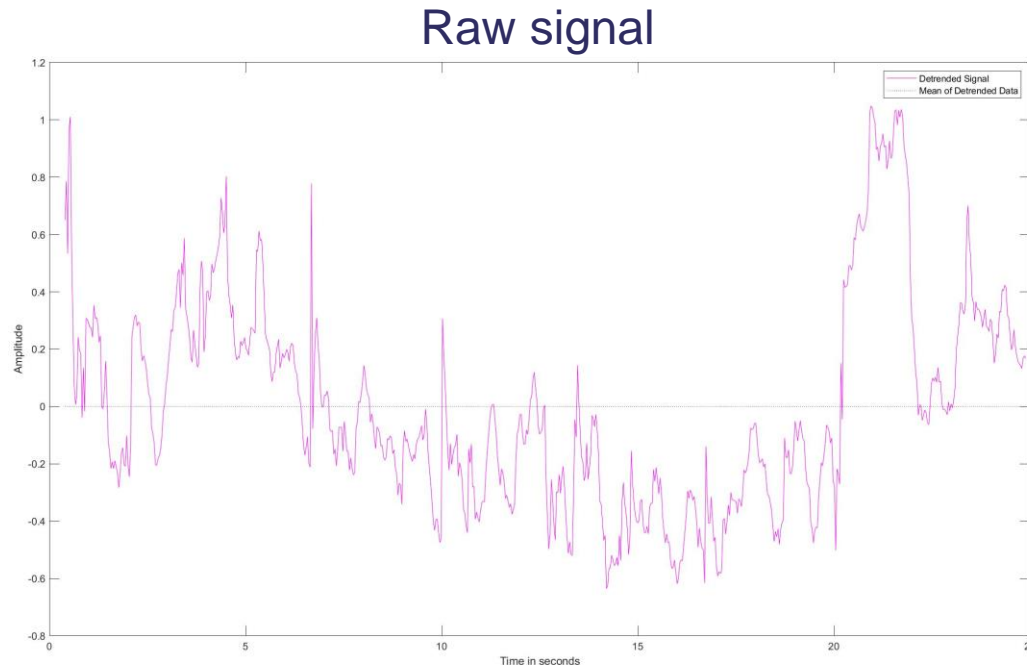


## Low-pass filtering: “Smoothing”



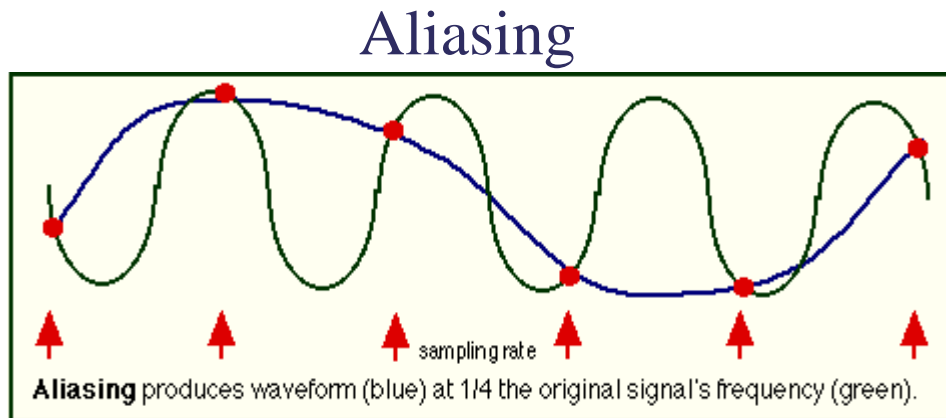
# Edge Artefacts of Filters

- Filtering artefacts occur at signal discontinuities, e.g. at the beginning and the end of the data.
- Thus, filter the “longest possible data segment”, ideally the raw data as early as possible.
- If you have to filter epochs, consider filtering longer epochs than you actually need.
- Be careful with “effects” close to the border of epochs.



# Filtering and Downsampling: “Aliasing”

- Downsampling can lead to “aliasing” if the data are not filtered appropriately (Nyquist theorem):  
Filter at least below half of the sampling frequency before downsampling.



Also watch:

<https://www.youtube.com/watch?v=R-IVw8OKjvQ>

Thanks to Alessandro.

# **Spatial Data Decompositions: Spatial Filtering**

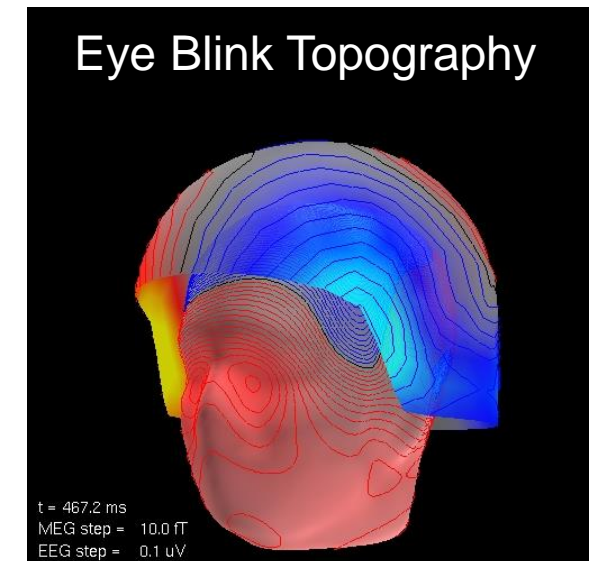
# Spatial Data Decompositions: SSP and ICA

If artefacts have characteristic topographies, several methods can be applied to remove (some) noise or extract signals:

- **SSP: Signal Space Projection** (needs pre-defined topographies)

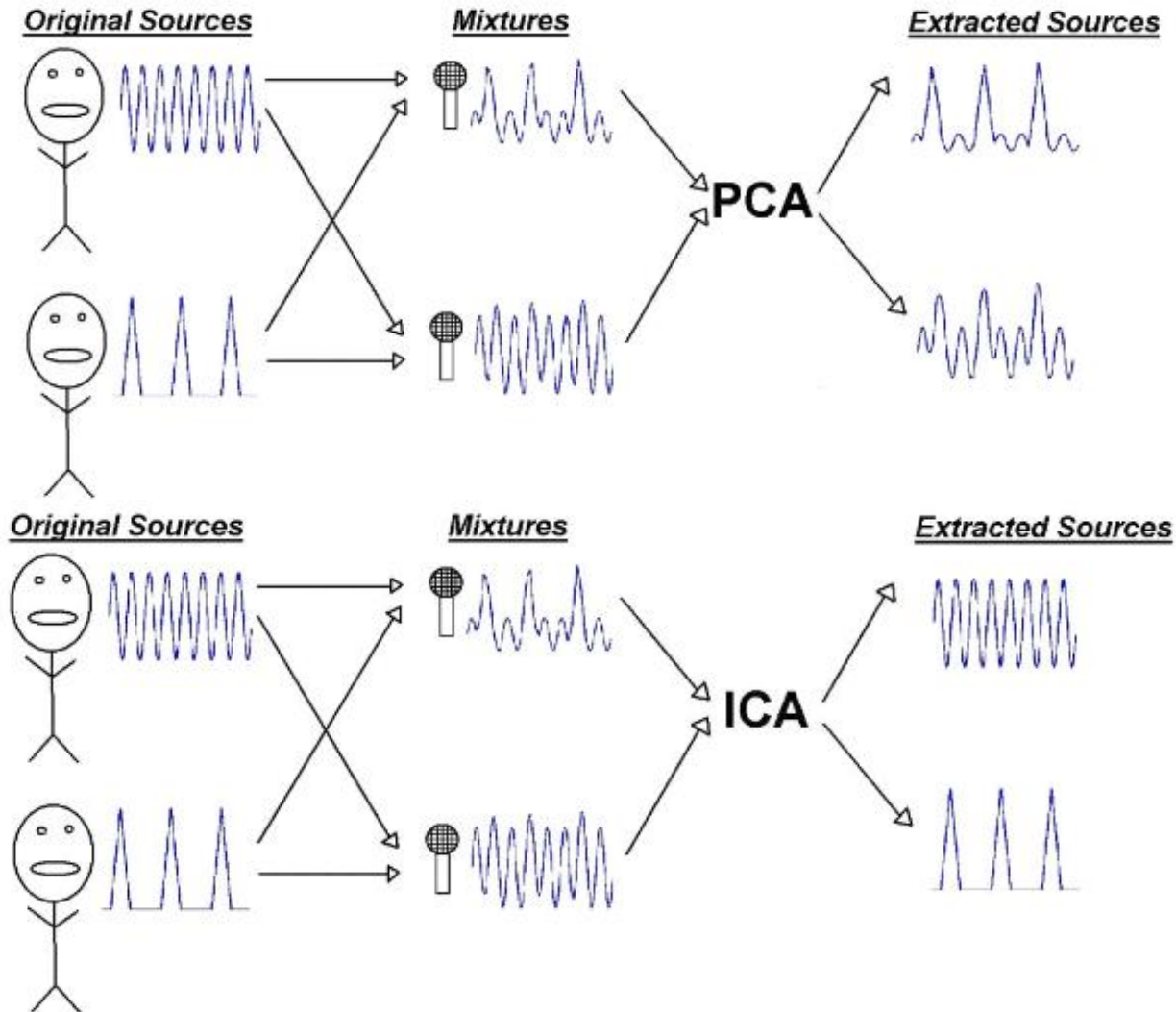
The following often go under the term “blind source separation”, because the topographies are not pre-defined, and found by the methods themselves (under certain assumptions):

- PCA: Principal Component Analysis
- SVD: Singular Value Decomposition
- **ICA: Independent Component Analysis**



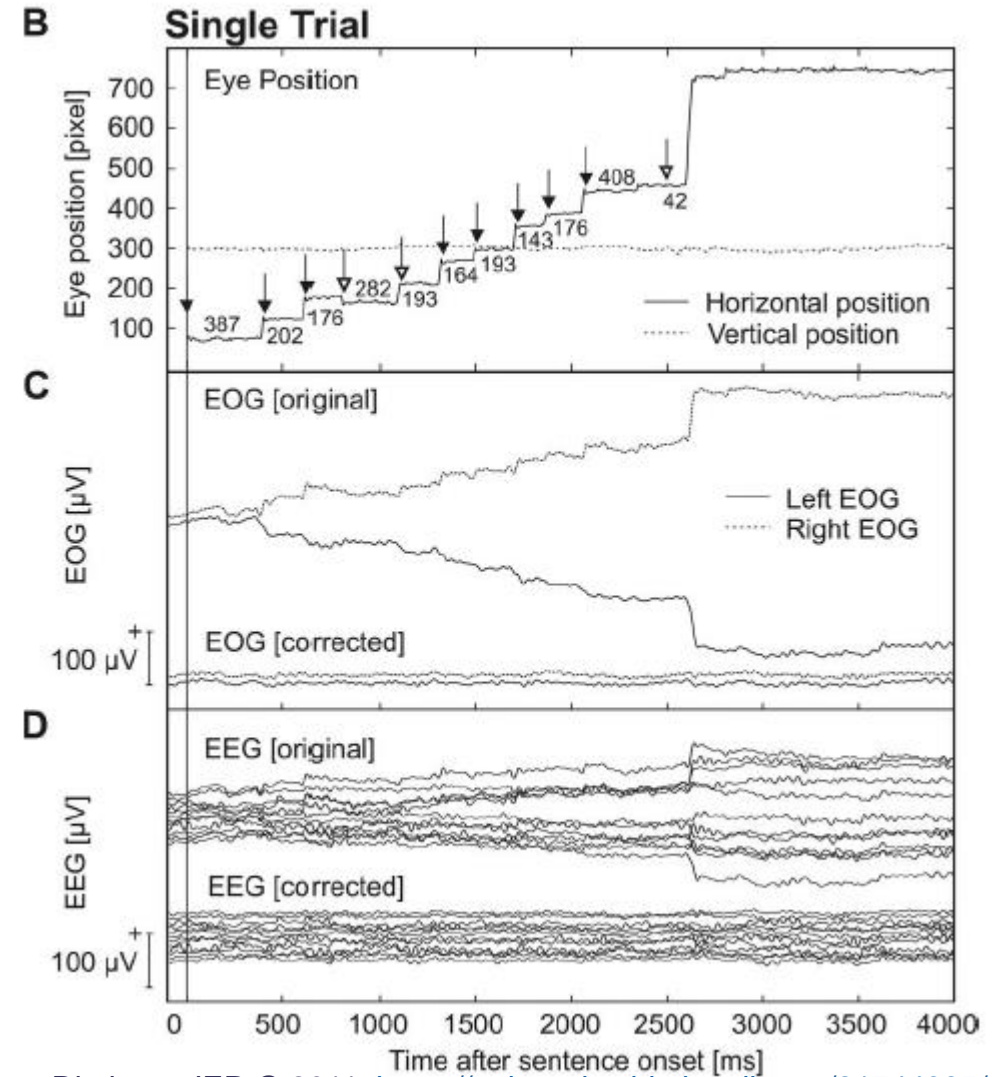
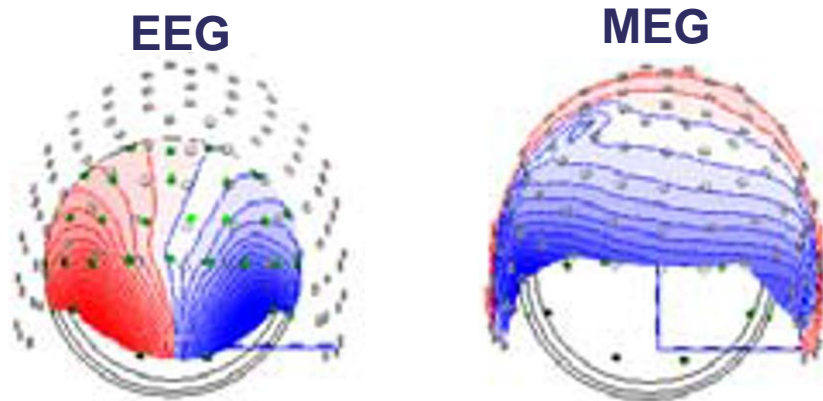
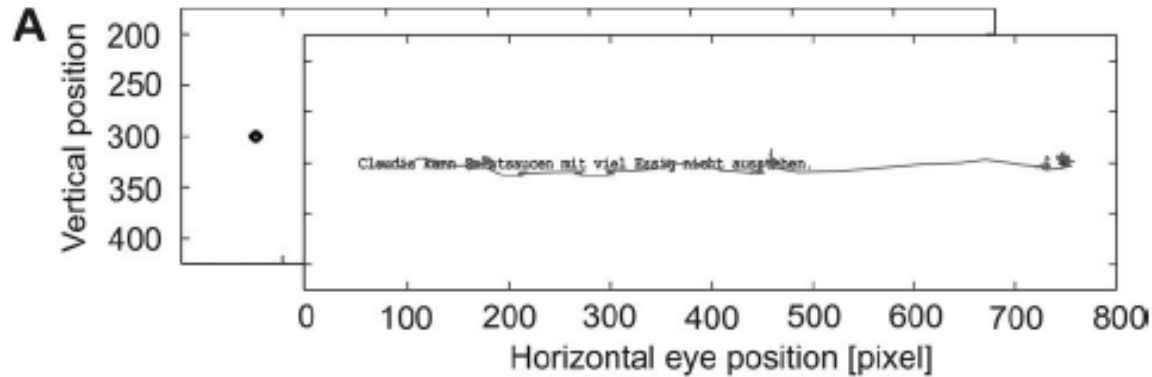
# Independent Component Analysis

Goal: (De-)mixing of sources in the cocktail party effect





# Tricky Example: Saccade Artefacts



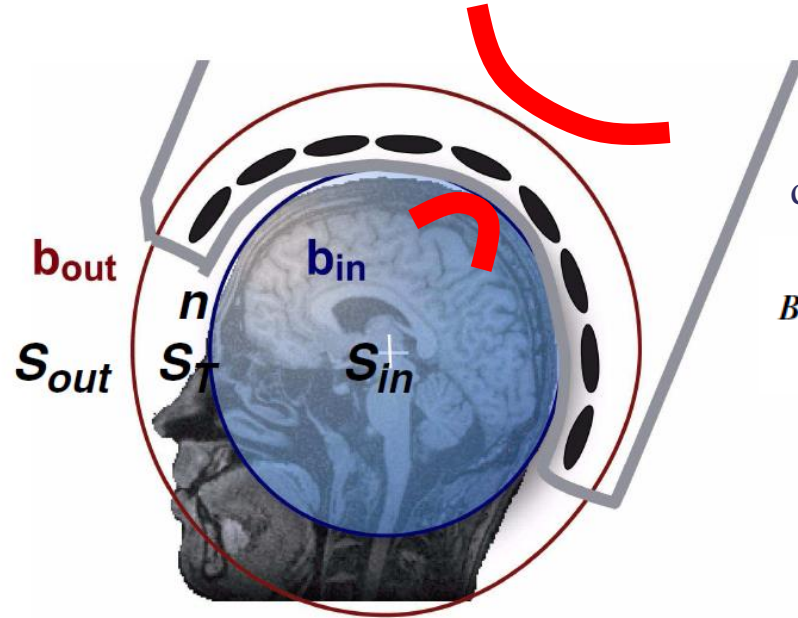
Dimigen, JEP-G 2011, <https://pubmed.ncbi.nlm.nih.gov/21744985/>

“Optimizing the ICA-based removal of ocular EEG artifacts from free viewing experiments”  
Dimigen, Neuroimage 2020, <https://www.sciencedirect.com/science/article/pii/S1053811919307086>



# “Maxfilter” – Maxwell Filtering

## Suppressing Signals From Distant Sources (MEG only)



$$\mathbf{b} = \mathbf{b}_{in} + \mathbf{b}_{out} + \mathbf{n}$$

### The mathematical basis of Maxfilter:

decomposition of magnetic fields into spherical harmonics

$$\mathbf{B}(r) = -\mu_o \sum_{n=1}^{\infty} \sum_{m=-n}^n \alpha_{nm} \frac{v_{nm}(\theta, \varphi)}{r^{n+2}} - \mu_o \sum_{n=1}^{\infty} \sum_{m=-n}^n \beta_{nm} r^{n-1} \omega_{nm}(\theta, \varphi).$$

$$v_{nm}(\theta, \varphi) = -(n+1)Y_{nm}e_r + \frac{\partial Y_{nm}}{\partial \theta}e_{\theta} + \frac{imY_{nm}}{\sin \theta}e_{\varphi},$$

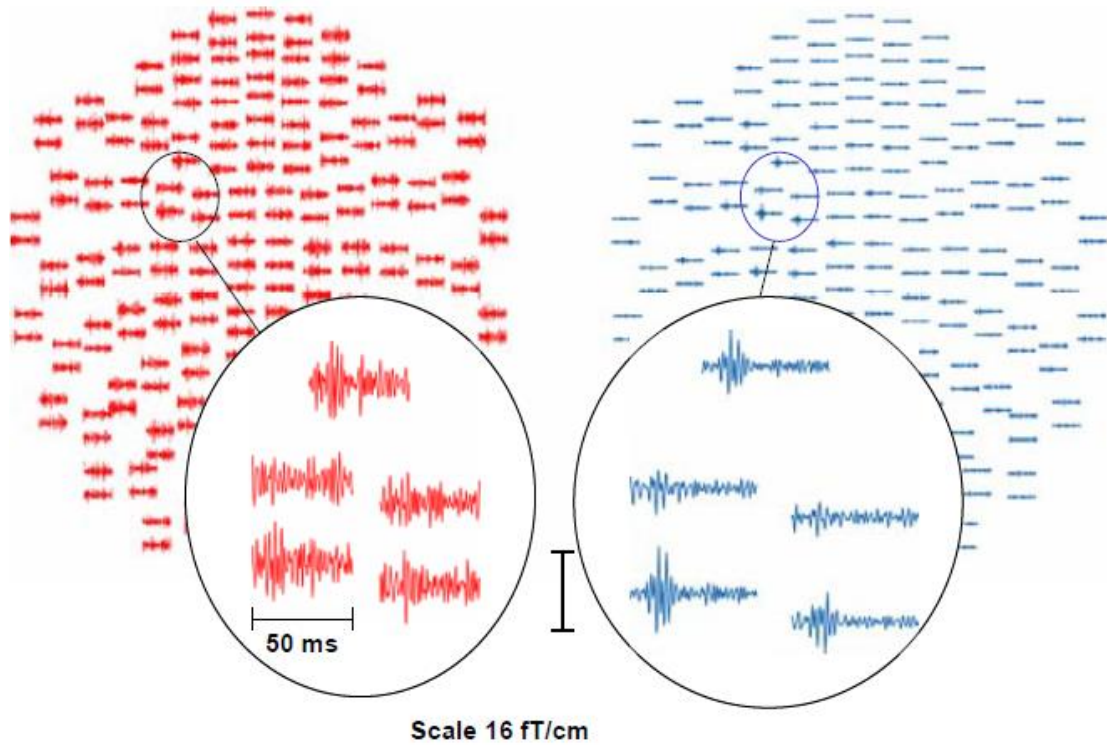
$$\omega_{nm}(\theta, \varphi) = nY_{nm}e_r + \frac{\partial Y_{nm}}{\partial \theta}e_{\theta} + \frac{imY_{nm}}{\sin \theta}e_{\varphi},$$

The measured magnetic field distribution is decomposed into “inside” (the helmet) and “outside” components, and the outside components are removed.

# Maxfilter – Signal Space Separation (SSS)

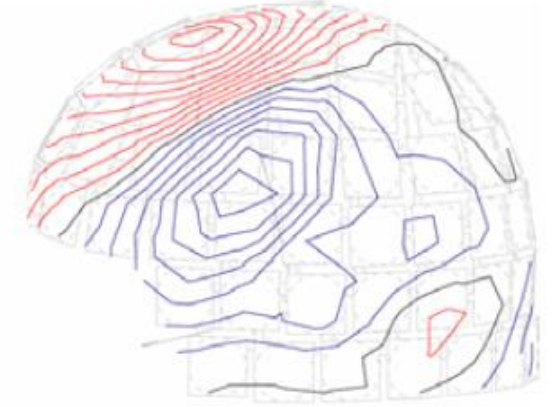
Without

With



Without

With



Original Field Map

SSS Reconstructed  
Field Map

Latency 20 ms  
 $Q = 2 \text{ nAm}$

# Maxfilter Software

## **Software shielding (Signal Space Separation, SSS)**

By subtracting the outer SSS components from measured signals, the program suppresses artifacts from distance sources.

## **Automated detection of bad channels**

By comparing the reconstructed sum with measured signals, the program can automatically detect if there are MEG channels with bad data that need to be excluded from Maxwell-filtering.

## **Spatio-temporal suppression of artifacts (“-st”)**

By correlation the time courses of SSS artefact components with the cleaned signal, the program can identify and suppress further artefacts that arise close to the sensor array.

**Notch Filter** to remove 50/60 Hz line noise.

## **Transformation of MEG data between different head positions (“-trans”)**

By transforming the inner components into harmonic amplitudes (i.e. virtual channels), MEG signals in a different head position can be estimated easily.

## **Compensation of disturbances caused by head movements (“-movecomp”)**

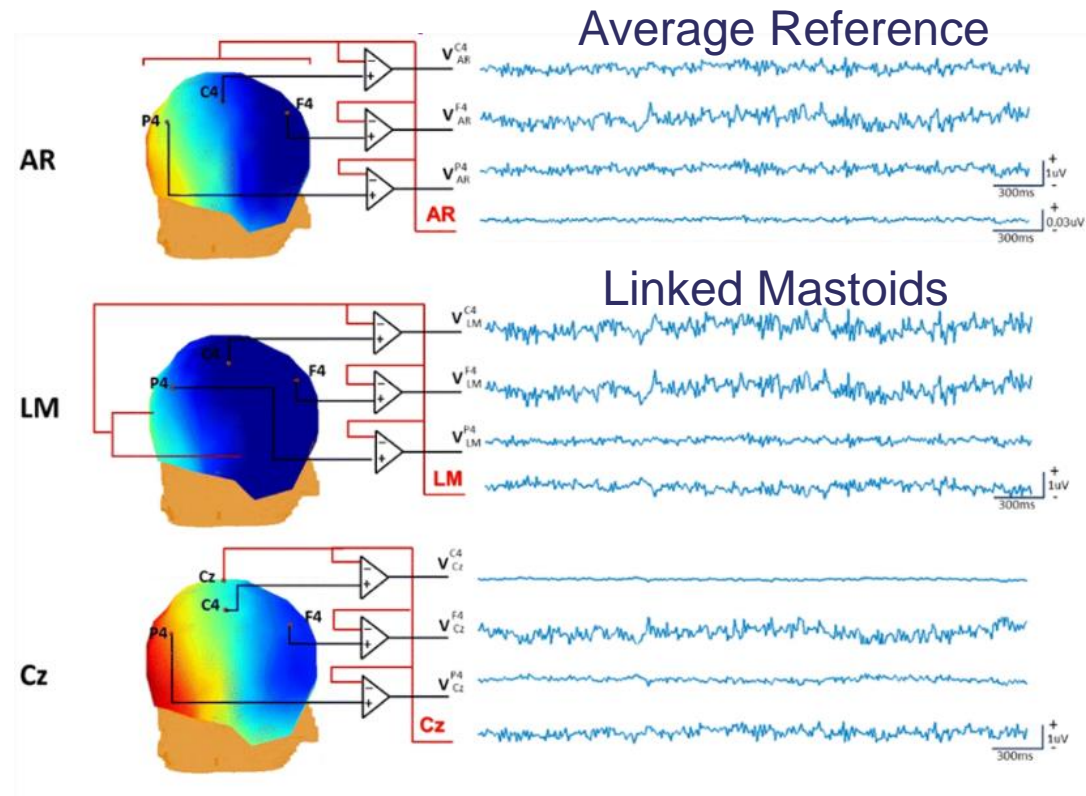
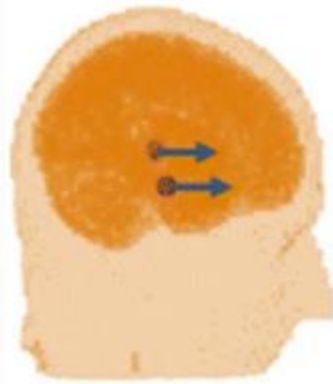
By extracting head position indicator (HPI) signals applied continuously during a measurement, the data transformation capability is utilized to estimate the corresponding MEG signals in a static reference head position.





# EEG only: Choice of reference site

Data from  
two simulated dipoles



The choice of reference changes time course and topography. For high-density recordings (> 65 channels), average reference is recommended. Note: Source estimates do not depend on the reference.



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# Thank you