

Implementation and validation of an Oxygen Exchange model coupled with multiple physics

life^x project

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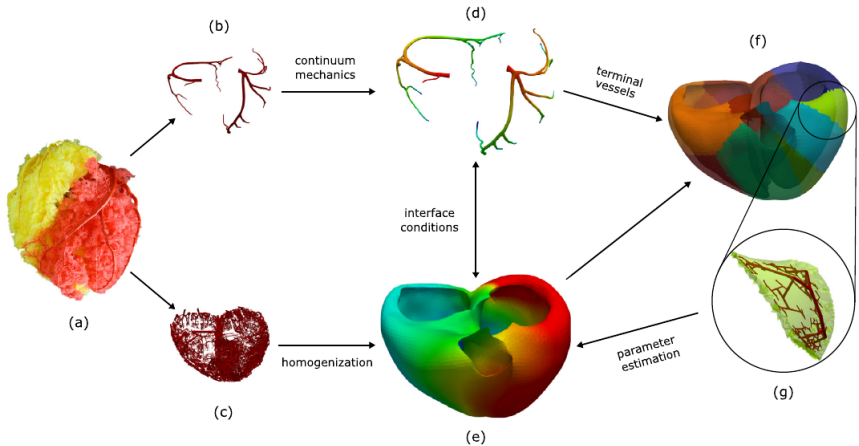


Figure: (a) Cast of Coronary Arteries, source Wikipedia; (b) epicardial vessels; (c) intramural vessels; (d) 3D blood flow dynamics model inside coronary domain (pressure depicted); (e) porous media flow model inside myocardial domain (pressure depicted); (f) myocardium partitioned into different perfusion regions; (g) example of generated intramural vascular network inside a perfusion region. Source: [3].

$$\frac{\partial}{\partial t} \text{PO}_2^i + \nabla \cdot (\text{PO}_2^i \psi_i^{-1} \hat{\mathbf{u}}_i) = n\alpha [\text{Hb}^*] k_- \left(\text{SO}_2^i - (1 - \text{SO}_2^i) \left(\frac{\text{PO}_2^i}{\text{PO}_2^{50}} \right)^n \right)$$

$$+ \psi_i^{-1} \hat{\phi}_{i-1,i} \text{PO}_2^{i-1} - \psi_i^{-1} \hat{\phi}_{i,i+1} \text{PO}_2^i \\ - \psi_i^{-1} \tilde{P} \left(\text{PO}_2^i - \text{PO}_2^m \right) \delta_{i3}$$

$$\frac{\partial}{\partial t} \text{SO}_2^i + \nabla \cdot (\text{SO}_2^i \psi_i^{-1} \hat{\mathbf{u}}_i) = -k_- \left(\text{SO}_2^i - (1 - \text{SO}_2^i) \left(\frac{\text{PO}_2^i}{\text{PO}_2^{50}} \right)^n \right)$$

$$+ \psi_i^{-1} \hat{\phi}_{i-1,i} \text{SO}_2^{i-1} - \psi_i^{-1} \hat{\phi}_{i,i+1} \text{SO}_2^i$$

$$\frac{\partial}{\partial t} \text{PO}_2^m = \psi_m^{-1} \tilde{P} (\text{PO}_2^3 - \text{PO}_2^m) - \xi_0 \left(1 + \frac{\text{PO}_2^{m,50}}{\text{PO}_2^m} \right)^{-1}$$

$$\Lambda_{\text{O}_2}^{\text{del}} = \frac{1}{T|\Omega|} \int_0^T \int_{\Omega} \tilde{P} \alpha^{-1} (\text{PO}_2^3 - \text{PO}_2^m)$$

$$\Lambda_{\text{O}_2}^{\text{cons}} = \frac{1}{T|\Omega|} \int_0^T \int_{\Omega} \psi_m \xi_0 \alpha^{-1} \left(1 + \frac{\text{PO}_2^{m,50}}{\text{PO}_2^m} \right)^{-1}$$

We can define the total oxygen concentration as $[\text{O}_2^*]^i := n[\text{Hb}^*] \text{SO}_2^i + \alpha^{-1} \text{PO}_2^i$ getting the reduced model

$$\begin{aligned} \frac{\partial}{\partial t} [\text{O}_2^*]^i + \nabla \cdot ([\text{O}_2^*]^i \psi_i^{-1} \hat{\mathbf{u}}_i) &= \psi_i^{-1} \hat{\phi}_{i-1,i} [\text{O}_2^*]^{i-1} - \psi_i^{-1} \hat{\phi}_{i,i+1} [\text{O}_2^*]^i \\ &\quad - \psi_i^{-1} \tilde{P} \alpha^{-1} \left((g^{-1}([\text{O}_2^*]^i) - \text{PO}_2^m) \right) \delta_{i3} \end{aligned}$$

$$\begin{aligned} \frac{\partial}{\partial t} \text{PO}_2^m &= \psi_m^{-1} \tilde{P} \left(g^{-1}([\text{O}_2^*]^3) - \text{PO}_2^m \right) \\ &\quad - \tilde{\xi}_0 \left(1 + \frac{\text{PO}_2^{50}}{\text{PO}_2^m} \right)^{-1} \end{aligned}$$

$$\Lambda_{\text{O}_2}^{\text{del}} = \frac{1}{T|\Omega|} \int_0^T \int_{\Omega} \tilde{P} \alpha^{-1} (g^{-1}([\text{O}_2^*]^3) - \text{PO}_2^m)$$

$$\Lambda_{\text{O}_2}^{\text{cons}} = \frac{1}{T|\Omega|} \int_0^T \int_{\Omega} \psi_m \tilde{\xi}_0 \alpha^{-1} \left(1 + \frac{\text{PO}_2^{m,50}}{\text{PO}_2^m} \right)^{-1}$$

Uncoupled problem

$$\hat{\mathbf{u}}_3 = \mathbf{0}$$

$$\hat{\phi}_{2,3} = \Phi \sin \left(\pi \frac{t \bmod T_{HB}}{T_F} \right)^4 1((t \bmod T_{HB}) < T_F)$$

$$\hat{\phi}_{3,4} = \hat{\phi}_{3,\text{veins}}(t) = \hat{\phi}_{2,3}(t)$$

where $\Phi = 0.05 \text{ s}^{-1}$ is the flux magnitude, $T_{HB} = 0.8 \text{ s}$ is the period of a heart beat and $T_F = 0.6 \text{ s}$ is the duration of the simulated flux.

Coupled problem

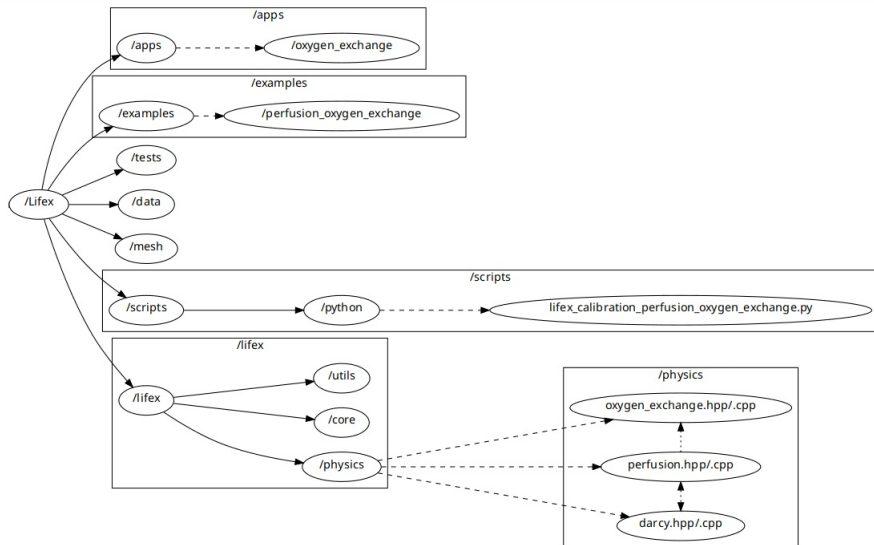
$$\hat{\mathbf{u}}_3 = -K_3 \nabla p_3$$

$$\hat{\phi}_{2,3} = \beta_{23}(p_3 - p_2)$$

$$\hat{\phi}_{3,4} = \hat{\phi}_{3,\text{veins}} = \gamma(p_3 - p_{\text{veins}})$$

where K_3 is the permeability tensor of the 3rd compartment, $\beta_{2,3}$ and γ are the inter-compartment pressure-coupling coefficients and p_{veins} is veins pressure.

$$\begin{aligned}
& \int_{\Omega} \frac{[\text{O}_2^*]^{3,k+1}}{\Delta t} v_h d\omega - \int_{\Omega} \mu \nabla [\text{O}_2^*]^{3,k+1} \nabla v_h d\omega \\
& - \int_{\Omega} [\text{O}_2^*]^{3,k+1} \psi_3^{-1} \hat{\mathbf{u}}_3 \cdot \nabla v_h d\omega + \int_{\Omega} \psi_3^{-1} \hat{\phi}_{3,4} [\text{O}_2^*]^{3,k+1} v_h d\omega \\
& = \int_{\Omega} \frac{[\text{O}_2^*]^{3,k}}{\Delta t} v_h d\omega + \int_{\Omega} \psi_3^{-1} \hat{\phi}_{2,3} [\text{O}_2^*]^{2,k+1} v_h d\omega \\
& - \int_{\Omega} \psi_3^{-1} \tilde{P}_\alpha^{-1} \left(g^{-1} \left([\text{O}_2^*]^{3,k} \right) - \text{PO}_2^{m,k} \right) v_h d\omega \quad \forall v_h \in X_h \\
\frac{\text{PO}_2^{m,k+1}}{\Delta t} & = \frac{\text{PO}_2^{m,k}}{\Delta t} + \psi_m^{-1} \tilde{P} \left(g^{-1} \left([\text{O}_2^*]^{3,k} \right) - \text{PO}_2^{m,k} \right) \\
& - \tilde{\xi}_0 \left(1 + \frac{\text{PO}_2^{50}}{\text{PO}_2^{m,k}} \right)^{-1}
\end{aligned}$$



```
module load gcc-glibc/11 dealii vtk
```

```
namespace lifex
{
    OxygenExchange::OxygenExchange(const std::string &subsection,
                                    const bool &standalone_)
        : CoreModel(subsection)
        , standalone(standalone_)
        , triangulation(std::make_shared<utils::MeshHandler>(
            prm_subsection_path,
            mpi_comm,
            std::initializer_list<utils::MeshHandler::GeometryType>←
                >(
                    {utils::MeshHandler::GeometryType::File,
                     utils::MeshHandler::GeometryType::Hypercube})))
        , fe_scalar(1)
        , linear_solver(prm_subsection_path + " / Linear solver",
                        {"CG", "GMRES", "BiCGStab"},
                        "GMRES")
        , block_preconditioner(prm_subsection_path +
                                " / Block preconditioner",
                                system_matrix)
        , csv_writer(mpi_rank == 0)
    {}
}
```


- We override the following base methods

```
declare_parameters()  
parse_parameters()  
run()
```

- To build some non-default set of parameters, we used `config/nondefault.json` file inside our app and example
- The `run` method calls in sequence different methods, depending on the spatial dimension
- To contain the 3D model solutions we used `LinAlg::MPI::BlockVector` data structures

```
LinAlg::MPI::BlockVector  
  c_O2_star; ///< [O2*] solution vector with ghost entries.  
LinAlg::MPI::BlockVector  
  P02_muscle; ///< P02_muscle solution vector with ghost ↔  
  entries.
```

- To handle the nonlinearity of the problem we used a look-up table based on a `std::map<double, double> g_inv_table` as it follows

```
/// Inverse of g.
double
g_inv(const double &c_O2_star) const
{
    auto p = g_inv_table.lower_bound(c_O2_star);
    double y2 = p->first;
    double x2 = p->second;
    // undefined behavior for prev if p = table.begin()
    double y1 = std::prev(p, 1)->first;
    double x1 = std::prev(p, 1)->second;
    return ((x2 - x1) / (y2 - y1)) * (c_O2_star - y1) + x1;
}
```

- We declared the class `Perfusion` as friend of `OxygenExchange` for coupling reason

```
class OxygenExchange : public CoreModel
{ public: // ...
    friend class Perfusion;
```

DarcyLinear

$p_3, p_2, p_{veins}, K_3, \beta_{2,3}$

OxygenExchange

$\phi_{2,3}, \phi_{3,veins}, \hat{\mathbf{u}}_3 = -K_3 \nabla p_3$

```
void
Perfusion::update_oxygen_exchange()
{
    oxygen_exchange->set_flux_darcy(darcy->get_gamma(),
                                     darcy->get_p_veins(),
                                     darcy->get_beta_23(),
                                     darcy->get_p_owned());
    oxygen_exchange->set_p_3_owned(darcy->get_p_owned());
}
```

```
grad_p_3 =
    std::make_unique<QuadratureFEMGradient>(
        p_3,
        dof_handler_scalar,
        *quadrature_formula);
```

```
/// Class in charge of computing outlet pressure for Network.
class BoundaryScalar : public ScalarBC
{
// ...
virtual double
value(const double & /*t*/)
{
    if (network_flow)
        return darcy->compute_average_subdomain_pressure(
            region, 0); // Always on first compartment
    else
        return 0;
};
```

```
/// Scalar source of the Darcy problem.
class ExampleScalarSource : public ScalarSource
{ // ...
virtual double
value(const Point<dim> &p, const unsigned int component = 0) ←
    const override
{
    double out = 0; // Output placeholder
    if (component == 0)
    { // Coupling with network flow
        out += values.at(material_id)
        // Other sources
        if (inlet_source_type == "Uniform")
            out += val;
        else if (inlet_source_type == "Sphere")
            { // ... }
        else if (inlet_source_type == "Sinusoidal")
            { // ... }
    }
    if (component == veins_compartment)
        out += venous_return;
    return out;
}
```

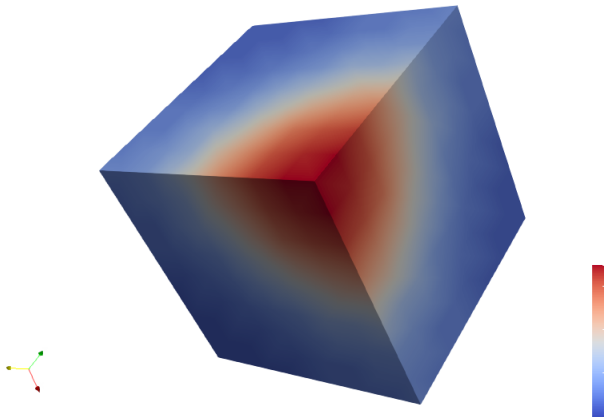
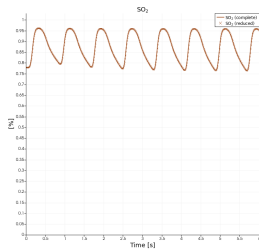
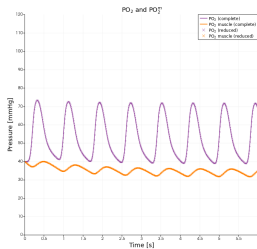


Figure: Spherical inlet for Darcy model

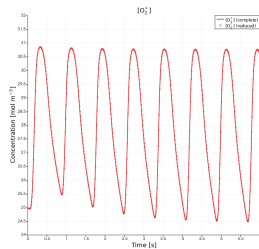
Comparison between complete and reduced 0D models



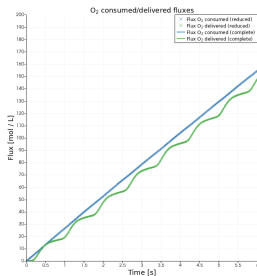
(a) SO_2



(b) PO_2 and PO_2^m



(c) $[\text{O}_2^*]$



(d) O_2 fluxes

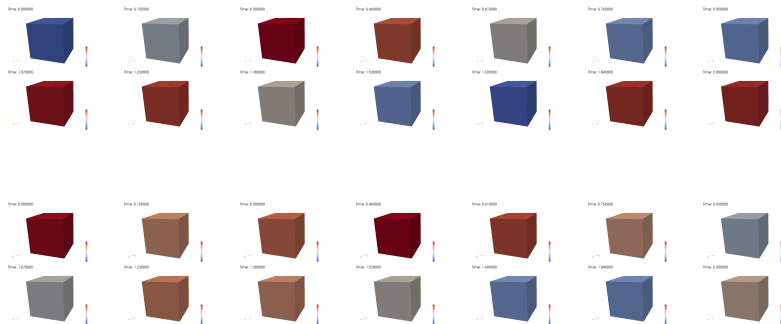
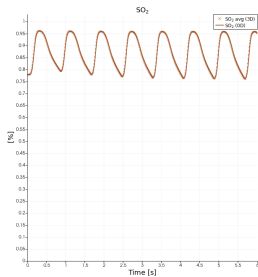
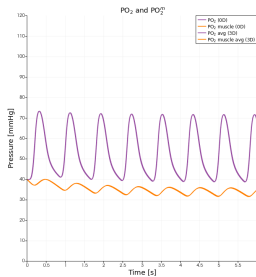


Figure: Results of 3D uncoupled model ($[O_2^*]$ and PO_2) with $t \in [0, 2]$ s, one frame every ~ 0.15 s.

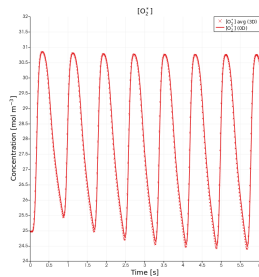
Comparison between reduced 3D and 0D models



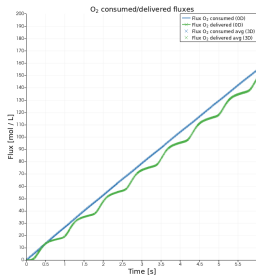
(a) SO_2



(b) PO_2 and PO_2^m



(c) $[\text{O}_2^*]$



(d) O_2 fluxes

Calibration of Darcy source

```
import numpy as np; import pandas as pd; from prettytable import PrettyTable

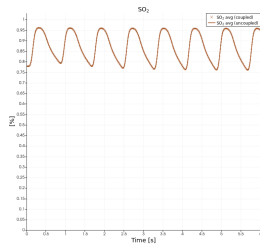
# Parameters
beta_12 = 2.6e-6; beta_23 = 3.62e-6; gamma = 1e-4
p_veins = 22.5 * 133; sphere_r = 5e-3; cube_l = 1e-2
sphere_vol = 1/8 * 4/3 * np.pi * sphere_r**3; cube_vol = cube_l**3

# Compute inlet source value
delta_p_12 = 24.66 * 133 # (from mmHg to Pa)
phi_01 = delta_p_12 * beta_12
value = phi_01 / (sphere_vol / cube_vol)

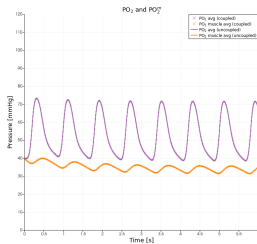
# Results
df = pd.read_csv('./results/perfusion.csv')
p_perf = np.array([df["p0_avg"][1], df["p1_avg"][1], df["p2_avg"][1]])
p = np.array([p_veins + gamma**(-1) * phi_01,
              p_veins + gamma**(-1) * phi_01 + beta_23**(-1) * phi_01,
              p_veins + gamma**(-1) * phi_01 + beta_23**(-1) * phi_01 + beta_12**(-1) * phi_01])
delta_p = (p_perf - p) / p_perf # ...
```

	Compartment 1	Compartment 2	Compartment 3
Avg pressure [Pa]	3077.77	5433.42	8713.2
Perfusion pressure [Pa]	8981.75	5548.0	3081.78
Delta [%]	0.66	0.02	-1.83

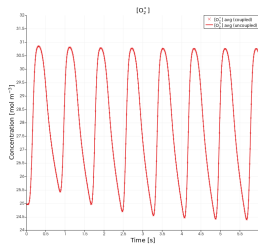
Comparison between coupled and 3D (uncoupled) models



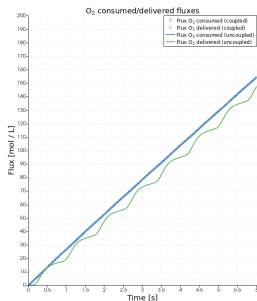
(a) SO_2



(b) PO_2 and PO_2^m

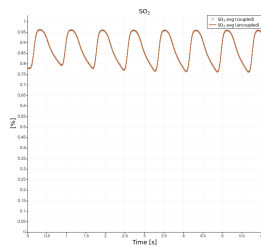


(c) $[\text{O}_2^*]$

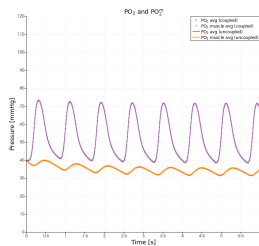


(d) O_2 fluxes

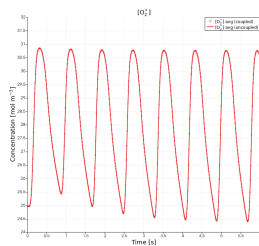
Validation of coupled 3D model - Smaller volume



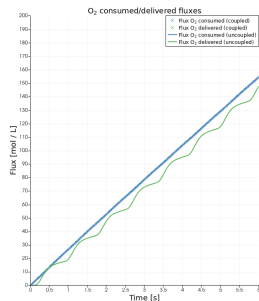
(a) SO_2



(b) PO_2 and PO_2^m

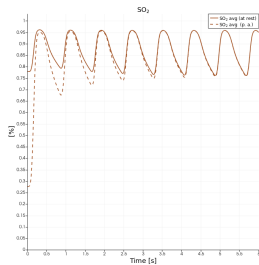


(c) $[\text{O}_2^*]$

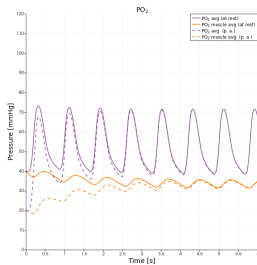


(d) O_2 fluxes

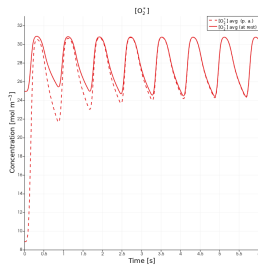
Effect of physical activity



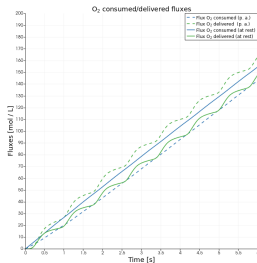
(a) SO_2



(b) PO_2 and PO_2^m

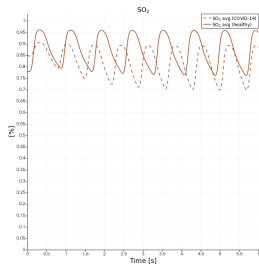


(c) $[\text{O}_2^*]$

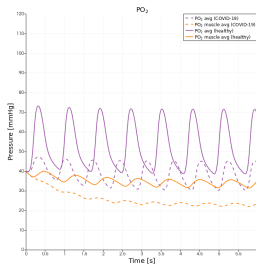


(d) O_2 fluxes

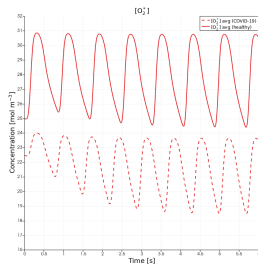
Effect of COVID-19 disease



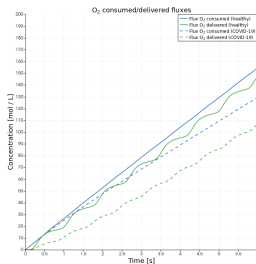
(a) SO_2



(b) PO_2 and PO_2^m

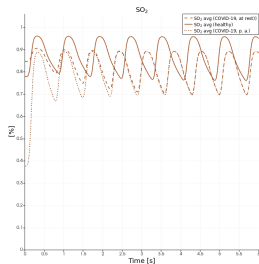


(c) $[\text{O}_2^*]$

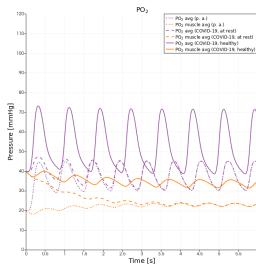


(d) O_2 fluxes

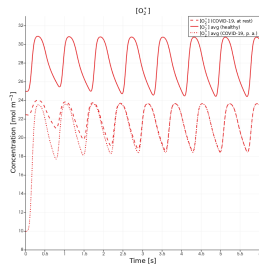
Effect of physical activity and COVID-19 disease



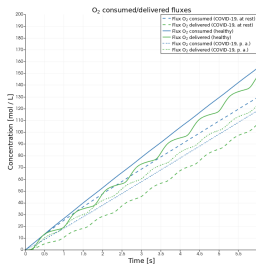
(a) SO_2



(b) PO_2 and PO_2^m

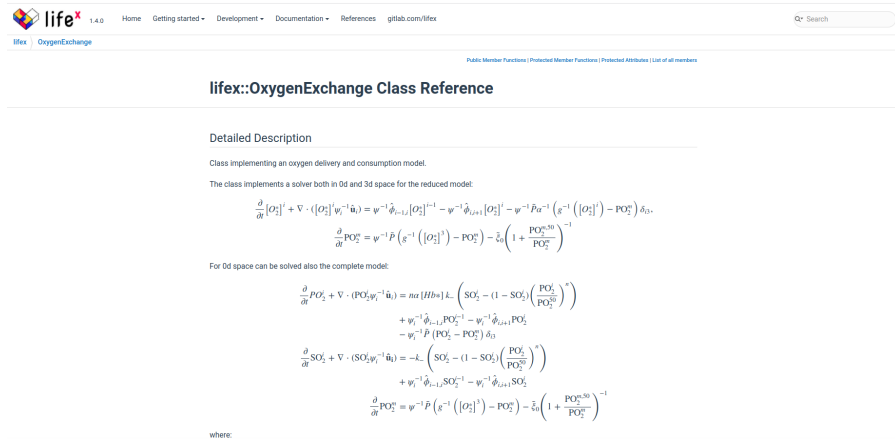


(c) $[\text{O}_2^*]$



(d) O_2 fluxes

https://gitlab.com/lifex/lifex/-/merge_requests/291



The screenshot shows the documentation for the `lifex::OxygenExchange` class. At the top, there is a navigation bar with the `lifex` logo (version 1.4.0) and links for Home, Getting started, Development, Documentation, References, and the gitlab.com repository. A search bar is also present. The main heading is `lifex::OxygenExchange Class Reference`. Below this, the 'Detailed Description' section states that the class implements an oxygen delivery and consumption model. It further explains that the class implements a solver for 0d and 3d space for a reduced model, providing two sets of equations. The first set of equations is for the 0d space, and the second set is for the complete model. The equations involve various variables like $[O_2]^i$, PO_2^n , SO_2 , and $PO_2^{n,SO}$, along with parameters like $\hat{\phi}$, \hat{P} , \hat{k}_- , and \hat{k}_+ . The page concludes with the word 'where:'.

lifex 1.4.0 Home Getting started Development Documentation References gitlab.com/lifex

lifex OxygenExchange

Public Member Functions | Protected Member Functions | Protected Attributes | List of all members

lifex::OxygenExchange Class Reference

Detailed Description

Class implementing an oxygen delivery and consumption model.

The class implements a solver both in 0d and 3d space for the reduced model:

$$\frac{\partial}{\partial t} [O_2]^i + \nabla \cdot ([O_2]^i \psi_i^{-1} \hat{\mathbf{u}}_i) = \psi_i^{-1} \hat{\phi}_{i-1,j} [O_2]^{i-1} - \psi_i^{-1} \hat{\phi}_{i,j+1} [O_2]^i - \psi_i^{-1} \hat{P} \alpha^{-1} \left(g^{-1} \left([O_2]^i \right) - PO_2^n \right) \delta_{i3},$$
$$\frac{\partial}{\partial t} PO_2^n = \psi^{-1} \hat{P} \left(g^{-1} \left([O_2]^3 \right) - PO_2^n \right) - \tilde{\zeta}_0 \left(1 + \frac{PO_2^{n,SO}}{PO_2^n} \right)^{-1}$$

For 0d space can be solved also the complete model:

$$\frac{\partial}{\partial t} PO_2^i + \nabla \cdot (PO_2^i \psi_i^{-1} \hat{\mathbf{u}}_i) = n \alpha [Hb*] k_- \left(SO_2 - (1 - SO_2) \left(\frac{PO_2^i}{PO_2^{n,SO}} \right)^{\kappa} \right) + \psi_i^{-1} \hat{\phi}_{i-1,j} PO_2^{i-1} - \psi_i^{-1} \hat{\phi}_{i,j+1} PO_2^i - \psi_i^{-1} \hat{P} (PO_2^i - PO_2^n) \delta_{i3}$$
$$\frac{\partial}{\partial t} SO_2 + \nabla \cdot (SO_2 \psi_i^{-1} \hat{\mathbf{u}}_i) = -k_- \left(SO_2 - (1 - SO_2) \left(\frac{PO_2^i}{PO_2^{n,SO}} \right)^{\kappa} \right) + \psi_i^{-1} \hat{\phi}_{i-1,j} SO_2^{i-1} - \psi_i^{-1} \hat{\phi}_{i,j+1} SO_2^i$$
$$\frac{\partial}{\partial t} PO_2^n = \psi^{-1} \hat{P} \left(g^{-1} \left([O_2]^3 \right) - PO_2^n \right) - \tilde{\zeta}_0 \left(1 + \frac{PO_2^{n,SO}}{PO_2^n} \right)^{-1}$$

where:

Figure: OxygenExchange class documentation in life^x website



F. Regazzoni – *Oxygen Exchange model*, internal report, Politecnico di Milano (2020).



P. C. Africa, R. Piersanti, M. Fedele, L. Dede', A. Quarteroni – *life^x - heart module: a high-performance simulator for the cardiac function*, <https://arxiv.org/abs/2201.03303>, Politecnico di Milano (2022).



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