Verification and comparison of MIT-BIH arrhythmia database based on number of beats

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ABSTRACT

The ECG signal processing methods are tested and evaluated based on many databases. The most ECG database used for many researchers is the MIT-BIH arrhythmia database. The QRS-detection algorithms are essential for ECG analyses to detect the beats for the ECG signal. There is no standard number of beats for this database that are used from numerous researches. Different beat numbers are calculated for the researchers depending on the difference in understanding the annotation file. In this paper, the beat numbers for existing methods are studied and compared to find the correct beat number that should be used. We propose a simple function to standardize the beats number for any ECG PhysioNet database to improve the waveform database toolbox (WFDB) for the MATLAB program. This function is based on the annotation's description from the databases and can be added to the Toolbox. The function is removed the non-beats annotation without any errors. The results show a high percentage of 71% from the reviewed methods used an incorrect number of beats for this database.

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1. INTRODUCTION

The electrocardiogram (ECG) was generally used for the observation of cardiac physiology as a cost-effective and non-invasive process. For the cardiologist to diagnose cardiac diseases, the ECG signal shows heart functionality. The ECG field is developed significantly, considering the most common death is generally from cardiovascular diseases [1]. Many applications are based on the ECG signal, such as measuring the heart-rate, biometric-identification, movement-recognize, and diagnosing-abnormality [2].

Generally, the first ECG standard material available for testing and performance evaluation is the MIT-BIH arrhythmia database [3]. It played together with the American Heart Association (AHA) database an interesting role in stimulating manufacturers of arrhythmia analyzers to compete on the basis of objectively measurable performance. The value of common databases for basic research and medical device development and evaluation is attributed to the MIT-BIH arrhythmia database. The MIT-BIH has comprised variable ECG signals with a variable: noise, artifacts, beat types, and wave shapes. A 48-records with two channels for each ECG-signal and an annotation file are included. These signals are recording from 25 men and 22 women for a half-hour period at 360 samples per second. The database has been annotated with 112,647 annotations, and these annotations have been verified [3]. It has been classified into two main annotation categories: the beats and the non-beats. The beat annotations for the MIT-BIH arrhythmia database consist of 15 subtypes, and the non-beats annotations consist of 24 subtypes, as shown in Table 1.

The beat type consists of 14 classified beats types and one unclassified beats type. The beats annotations are occurring for any type of QRS waves in ECG-signal. Therefore, this database is widely used for testing, performance evaluating, and learning for QRS-detection methods. In general, the databases are used to evaluate any new algorithm's performance before implementing it in devices for many applications. So, any errors for this evaluation will cause an error in the device decision. In biomedical applications like QRS-detection, which is substantial for many ECG monitoring devices, the detecting errors for these devices may affect doctor's diagnosis and treatment depending on these devices. So, verifying the database for these applications will improve the doctor's decision.

Table 1. The description of beat and non-beat annotations for MIT-BIH arrhythmia database

Beat an	notations	Non-beat a	nnnotations
Code	Description	Code	Description
N	Normal beat	[Start of ventricular flutter/fibrillation
L	Left bundle branch block beat	!	Ventricular flutter wave
R	Right bundle branch block beat]	End of ventricular flutter/fibrillation
A	Atrial premature beat	X	Non-conducted P-wave (blocked APC)
a	Aberrated atrial premature beat	(N	Normal sinus rhythm
J	Nodal (junctional) premature beat	(P	Paced rhythm
S	Supraventricular premature or ectopic beat (atrial or nodal)	(B	Ventricular bigeminy
V	Premature ventricular contraction	(VT	Ventricular tachycardia
F	A fusion of ventricular and normal beat	(T	Ventricular trigeminy
e	Atrial escape beat	(SVTA	Supraventricular tachyarrhythmia
j	Nodal (junctional) escape beat	(IVR	Idioventricular rhythm
E	Ventricular escape beat	(NOD	Nodal (A-V junctional) rhythm
/	Paced beat	(AFIB	Atrial fibrillation
f	A fusion of paced and normal beat	(AFL	Atrial flutter
Q	Unclassifiable beat	(VFL	Ventricular flutter
		(AB	Atrial bigeminy
		(PREX	Pre-excitation (WPW)
		(BII	2° heart block
		(SBR	Sinus bradycardia
			Isolated QRS-like artifact
		~	Change in signal quality
		":TS	Tape slippage
		":PSE	Pause
		":MISSB	Missed beat

Until now, more than two thousand works cited the MIT-BIH arrhythmia database. It is unique in terms of arrhythmia classification since it offers five arrhythmia standards groups [2]. The QRS detection methods are essential for most of the cited works, including arrhythmia detection, classification, and diagnosing applications. Depending on this database, many QRS detection algorithms have been developed, tested, and evaluated. The QRS detection algorithms are based on the beats annotations in the database signals for testing and evaluation. These beats are used as learning data for the methods depending on the learning technique.

Many researchers used MATLAB for algorithm implementation based on the waveform database (WFDB) Toolbox [4]. This Toolbox consists of the functions that are used for reading, writing, and signals processing the files of PhysioNet databases. The MIT-BIH arrhythmia is one of the PhysioNet databases which contains data and annotations files. The WFDB is used to extract the ECG-signals and these annotations from the MIT-BIH arrhythmia database for all records. It can extract one type of beats or nonbeats annotations or extract all annotations without any filter. So, it is not easy to extract all beat annotations only, which is leads to errors from reading the non-beat annotations. When reviewing the existing methods that used the MIT-BIH arrhythmia database, we noted that not all these methods are considered the same number of beats for the same database records. Also, this difference affects even slightly the evaluation results used to compare the performance of the methods.

This work will study the reasons for reading different numbers of beats and methods comparison with correction and verification. Furthermore, a new function is designed to extract the correct beats and remove the non-beats annotations from the original database files based on WFDB Toolbox for MATLAB.

In section 2, the MIT-BIH arrhythmia database and its annotation types in detail are described. Section 3 present the proposed function that extracts the correct beat from the annotation files. Then, section 4 demonstrates the results and discussion for revising the existing methods with a comparison based on each method's beat number. Finally, in section 5, the conclusion is summarized.

2. MIT-BIH ARRHYTHMIA DATABASE

The MIT-BIH arrhythmia database is one of the most substantial ECG databases. Contrasting database signals, noise, and artifacts make it suitable for testing and evaluation. Moreover, the verified annotations files that contain the beats and non-beats types, as shown in Table 2 and Table 3. These tables show the MIT-BIH arrhythmia database annotations for each record based on the PhysioNet annotations descriptions for beats and non-beats annotations. There are more than these annotation types, which are shown in other databases.

Table 2. MIT-BIH arrhythmia database beat annotations

			Table	2. IVI	11-DII	i airii	y tiiiii	ıa u	atabas	ic oca	t aiii	iotati	0113				m · 1
Record	Total	N	L	R	Α	a	J	S	V	F	e	j	E	/	f	Q	Total
No.	Anno-tations											,				`	Beats
100	2274	2239			33				1								2273
101	1874	1860			3											2	1865
102	2192	99							4					2028	56		2187
103	2091	2082			2												2084
104	2311	163							2					1380	666	18	2229
105	2691	2526							41							5	2572
106	2098	1507							520								2027
107	2140								59					2078			2137
108	1824	1739			4				17	2		1					1763
109	2535		2492						38	2							2532
111	2133		2123						1								2124
112	2550	2537			2												2539
113	1796	1789				6											1795
114	1890	1820			10		2		43	4							1879
115	1962	1953															1953
116	2421	2302			1				109								2412
117	1539	1534			1												1535
118	2301			2166	96				16								2278
119	2094	1543							444								1987
121	1876	1861			1				1								1863
122	2479	2476															2476
123	1519	1515							3								1518
124	1634			1531	2		29		47	5		5					1619
200	2792	1743			30				826	2							2601
201	2039	1625			30	97	1		198	2		10					1963
202	2146	2061			36	19			19	1							2136
203	3108	2529			20	2			444	1						4	2980
205	2672	2571			3	-			71	11						•	2656
207	2385	23/1	1457	86	107				105				105				1860
208	3040	1586	1437	00	107			2	992	373			105			2	2955
209	3052	2621			383			_	1	313						2	3005
210	2685	2423			363	22			194	10			1				2650
212	2763	923		1825		22			194	10			1				2748
212	3294	2641		1023	25	3			220	362							3251
214	2297	2041	2003		23	3			256	1						2	2262
215	3400	3195	2003		3				164	1						2	3363
217	2280	244			3				162	1				1542	260		2208
217	2312	2082			7				64	1				1342	200		2154
219	2069	1954			94				04	1							2048
220					94				206								2048 2427
221	2462	2031			200		1		396			212					2427
222	2634	2062			208	1	1		472	1.4	16	212					2483
223	2643	2029			72	1			473	14	16						2605
228	2141	1688			3				362								2053
230	2466	2255		1051	1				1								2256
231	2011	314		1254	1				2								1571
232	1816	2222		397	1382				021			1					1780
233	3152	2230			7				831	11							3079
234	2764	2700	0077	70.50	2516	1.50	50	^	3	003	1.0	222	100	7020	002	22	2753
Total	112647	75052	8075	7259	2546	150	83	2	7130	803	16	229	106	7028	982	33	109,494

Each beat's annotation is a QRS-complex with different types as normal-beat or other beats. On the other hand, The Non-beat annotations are ventricular flutter wave, start/end of ventricular flutter, and starting for many types of rhythm like (sinus, paced, ventricular, supraventricular, atrial fibrillation, atrial flutter, and heart block). These are annotated ECG signal to show at this point one of the rhythms are starting. So, it is not a beats (QRS) annotation. The ventricular flutter (record 207) is excepted for many QRS-detection methods because it is defined on the ECG by a sinusoidal wave without a clear showing of the QRS-complex

wave and T wave. The QRS detection methods based on the MIT-BIH arrhythmia database use the beat annotation only because the non-beats annotations are not shown QRS waves for testing, evaluation, and learning.

The number of beats annotations are shown in Table 2 with (109,494 Beats) for all 48 records. This number should be a standard number of beats depending on the original database annotation details and the PhysioNet annotations descriptions for beats and non-beats types. Also, the QRS detection methods are excluded from the 472 ventricular flutter waves from record no. 207, because these waves are considered as non-beat annotations based on the annotation's description of PhysioNet as shown in Table 3.

Table 3. MIT-BIH arrhythmia database non-beat annotations

	Table 3. MIT-BIH arrhythmia database non-beat annotations														_											
Record	Total				.,	7	0	3	T		TA	R	OD	IB.	FL	FL	В	EX	П	3R		,	S	SE	SSB	TAIN DA
No.	Anno- tations	_			· ×	€	D	(I	2	, □	SV	5	ž	(AF	\overline{A}	\leq	Ą	(PREX	(B	(SBR	_	l	ST:"	":PSE	":MISSB	Total Non-Beats
100	2274					1																				1
101	1874					1															4	4				9 5
102	2192					2	3																			5
103	2091					1																6				7
104	2311					22	23															37				82
105	2691					1															30	88				119
106	2098					21		18	1	1												30				71
107	2140						1															2				3
108	1824				11	1															8	41				61
109	2535					1																2				3
111	2133					1																8				9
112	2550					1																10				11
113	1796					1																				1
114	1890					2					1										1	7				11
115	1962					1															6	2				9
116	2421					1																8				9
117	1539					1																3				4
118	2301				10	1																12				23
119	2094					49		37		17												4				107
121	1876					1																12				13
122	2479					1															2					3
123	1519					1																				1
124	1634					6				2		3	2									2				15
200	2792					70		71	7													43				191
201	2039				37					12	1		3	3								4				76
202	2146					3								4	1						2					10
203	3108					_			21	1				21	2						26	57				128
205	2672	_				7			6												1	2				16
207	2385	6	472	6		10		4	2		1	1				6					2	15				525
208	3040					27				26	1.0										8	24				85
209	3052					11		_	•		10			_							7	19				47
210	2685							5	2	1				9							1	17				35
212	2763					1		10	_												1	13				15
213	3294					22		19	2	10											_					43
214	2297					13			2	10											5	4	1			35
215	3400					3	22		2					2.4								30	2			37
217	2280				122	0	33	9	1					24							1	4		2	1	72
219	2312				133			2		1	0			10								4		3	1	158
220	2069					9			2	0	8			10								4				21
221	2462					22		1	2	8	4		2.1	12	40		2					12				35
222	2634					32		7	7	2	4		31	24	42		3					15				151
223	2643					11		7	7	3											24	10	2			38
228	2141					21		20										102			24	20	3			88
230	2466				2	104												103	_		1	2			427	210
231	2011				2	6													5	1		25			427	
232	1816					20		20	,	1										1	2	35				36
233	3152					36		28	6	1	1										2	0				73
234 Total	2764	6	472	6	102	2	60	221	61	92	1	1	26	107	15	6	2	102	5	1	122	8	6	2	120	11 3 3153
Total	112647	Ü	4/2	υ	193	230	00	ZZ I	01	03	20	4	30	10/	43	U	3	103	J	1	132	010	U	3	428	3133

3. HEARTBEATS FILTER FUNCTION

In this paper, a MATLAB function is designed to filter the annotations file for any PhysioNet databases included the MIT-BIH arrhythmia. The function removes the non-beat annotation shown in Table 3 so, the annotations file will contain the beat annotation only shown in Table 2. On the other hand, the existing

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MATLAB-WFDB function (rdann) reading the annotations file can read all annotations or one annotation. So, rdann cannot filter the annotation by beats or non-beats type; for this reason, the function with new features was proposed with new features to filter the data correctly without any errors.

This function is simple, but it is important to standardize the beats number for any researcher that are used PhysioNet databases. This function can be added to the MATLAB-WFDB toolbox to simply filtered the annotations files by removing the non-beat annotations precisely with the standard values. The function read and search all annotations data files for each record, as shown in Figure 1. If the annotation is one of the non-beat types, this annotation will be removed from the annotation data. Also, it has to be used for any PhysioNet database to extract the beat annotation by removing the non-beat annotations used to prepare the data for many applications, including QRS-detection methods.

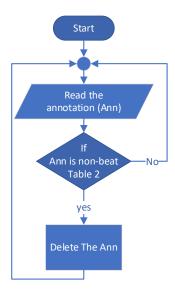


Figure 1. The function flowchart

4. THE COMPARISON AND VERIFICATION RESULTS WITH DISCUSSION

The work focuses on the verification and comparison of the MIT-BIH arrhythmia database used for the QRS-detection algorithm. The proposed heartbeats filter function can apply to all MIT-BIH databases from the PhysioNet site. The reviewed QRS-detection methods are not using the same number of heartbeats for the MIT-BIH arrhythmia database. This number should be standard for this database because it depends on the original database's beats number. Simultaneously, not all the QRS-detection methods are considering the same number of beats for the same database records. The revision for the existing QRS-detection methods using the MIT-BIH arrhythmia database has summarized the errors for these methods based on the beats for records shown in Table 4 (see in Appendix). The incorrect records are indicated by bold, the Total (T), and Errors (E) in this table. The methods should use the same number of beats without any difference, but the errors are occurring by researchers. All the reviewed methods are revised, compared, and verified based on beats number for each database record. Table 5 summarizes the total beats number, total error per record, and total error per database for different methods to evaluate these methods' incorrectness.

The total number of beats for the MIT-BIH arrhythmia database used from the reviewed methods is calculated; this number should be 109,494 heartbeats for all database records, as shown in section 2. The beat errors for these methods compared to the correct number of beats for this database are determined to find the number of methods that used the correct beat's value. Also, the other methods contained errors start from 1 beat to 1400 beats for the overall database. Table 5 shows the percentage of references number for each error per the total references that were reviewed. Moreover, it shows the total number of errors for each reference per each record (sum of the absolute values of errors) and the total number of errors for each reference per overall database, which takes a positive or negative value.

The beats errors per all data record up to 1400 beats and 29% of the total reviewed methods use the correct beats number. On the other hand, 71% are using incorrect beats number. Also, the number of incorrect methods is higher than the number of correct methods based on our comparison. So, we propose this study. Each record in the database for the reviewed methods has been studied for beats errors calculation.

Figure 2 describes the number of references that contain errors for each record. For each record, the percentage of the reference number that occurs error per all references is calculated to evaluate the record error reasons. The records error percentage is started from 53% for record no. 207 to 9% for records (102, 103, 112, 117, 119, 122, 123, and 230).

Table 5 and Figure 2 show the difference between these methods for the same records used from the same database. After the results are studied, the following obvious points are established:

- a. The correct number of the beats is 109,494 beats without adding or removing any data.
- b. The designed function extracts the correct heartbeats number of all records for the MIT-BIH arrhythmia database.
- c. If the beats number exceed the correct number:
 - Some non-beat annotations have been added and should be mentioned in the methods.
 - The data has been repeated for record and should be mentioned in the methods.
- d. If the beats number less than the correct number:
 - Some beat annotations have been removed and should be mentioned in the methods.
- e. This database contains some errors before digitalization and verification [1].
- f. The WFDB toolbox does not include the beats or non-beats filter for the (rdann) function that reads the annotations files.
- g. The copy and paste records beat numbers between the researchers without verification.
- h. A high number of annotation types (39 annotations) confuse the researchers.
- i. According to Figure 2, the most error occurs in record no. 207 because many researchers are counting the 472 ventricular flutter waves, but these waves are considered as non-beat annotations based on the annotation's description of PhysioNet.
- j. From Figure 2, records no. 209 is the second, and records no. 214 is the third most errors beats for the reviewed methods, but the number of errors is low and not exceeds eight beats and nine beats, respectively.
- k. According to Figure 2, the lowest error records (102, 103, 112, 117, 119, 122, 123, and 230) because these records contain the lowest non-beat annotations.

Table 5. Total beat annotations and errors for the reviewed methods

1 at	nemous				
References	Count of ref	Percentage ref	Total beats	Total errors per record	Total Errors per database
[5-24]	20	29%	109494	0	0
[25]	1	1%	109493	ĺ	-1
[26-31]	6	9%	109496	2	2
[32]	1	1%	109495	3	1
[33]	1	1%	109488	6	-6
[34]	1	1%	109488	6	-6
[35]	i	1%	109486	8	-8
[36]	1	1%	109481	13	-13
[37-39]	3	4%	109508	16	14
[40-42]	3	4%	109510	18	16
[43]	1	1%	109483	23	-11
[44]	1	1%	109488	36	-6
[45]	1	1%	109478	44	-16
[46]	1	1%	109443	51	-51
[47]	1	1%	109428	66	-66
[48]	i	1%	109328	166	-166
[49]	1	1%	109357	203	-137
[50]	i	1%	109255	239	-239
[51-56]	6	9%	109809	329	315
[57]	ĺ	1%	109788	348	294
[58]	1	1%	109267	357	-227
[59]	1	1%	109134	360	-360
[60]	1	1%	109097	423	-397
[61-63]	3	4%	109966	472	472
[64]	1	1%	109965	473	471
[65]	1	1%	109966	474	472
[66]	1	1%	109996	502	502
[67]	1	1%	109369	567	-125
[68]	1	1%	109985	579	491
[69]	1	1%	109663	603	169
[70]	1	1%	110159	665	665
[71]	1	1%	110008	738	514
[72]	1	1%	109036	1400	-458
Total	68	100%			

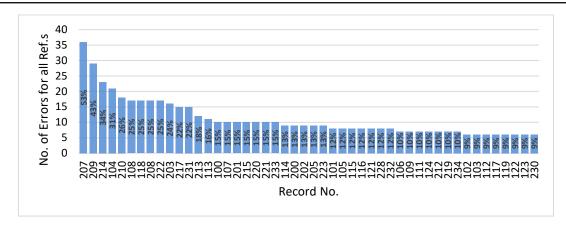


Figure 2. Records errors per overall references

5. CONCLUSION

This paper presented a method for finding the correct beats number for the MIT-BIH arrhythmia database with a comparison study and design a function for MATLAB to extract the correct values for any PhysioNet databases. In this way, the number of beats that are using by the researchers will be standards. The non-beat annotations affected the results of the QRS-detection methods in two ways. First, the proposed methods' evaluation accuracy is not calculated correctly because the number of database beats is incorrect. Second, the methods based on machine learning are trained depending on incorrect information. So, the learning operation was not proper, and the results of the methods are not correct. Most reviewed methods used an incorrect number of beats, 29% of researchers used the correct number, and 71% are used incorrect beats. The proposed function should be added to the MATLAB-WFDB Toolbox to filter the annotations files to remove the non-beat annotations correctly and extract the standard beat values. It can be used for any other programing language to read the annotations files from the PhysioNet databases like python.

APPENDIX

123 1518

124 1619

200 2601

1963 1963

2980 2980

2656 2656

1860 1862

100	2273	2273	2273	2273	2273	2273	2272	2272	2272	2273	2273	2273	2273	2273	2271	2273	2272
101	1865	1865	1865	1865	1865	1865	1865	1865	1865	1865	1865	1865	1865	1865	1864	1865	1864
102	2187	2187	2187	2187	2187	2187	2187	2187	2187	2187	2187	2187	2187	2187	2186	2187	2187
103	2084	2084	2084	2084	2084	2084	2084	2084	2084	2084	2084	2084	2084	2084	2083	2084	2084
104	2229	2229	2229	2229	2229	2229	2228	2228	2228	2229	2229	2229	2229	2230	2228	2229	2227
105	2572	2572	2572	2572	2572	2572	2572	2572	2572	2572	2572	2572	2572	2572	2571	2572	2555
106	2027	2027	2027	2027	2027	2027	2027	2027	2027	2027	2027	2027	2027	2027	2026	2027	2027
107	2137	2136	2137	2137	2137	2137	2136	2137	2137	2137	2137	2137	2137	2137	2136	2137	2135
108	1763	1763	1763	1763	1763	1763	1763	1763	1763	1774	1774	1760	1774	1763	1762	1763	1761
109	2532	2532	2532	2532	2532	2532	2532	2532	2532	2532	2532	2532	2532	2532	2531	2532	2532
111	2124	2124	2124	2124	2124	2124	2124	2124	2124	2124	2124	2124	2124	2124	2123	2124	2124
112	2539	2539	2539	2539	2539	2539	2539	2539	2539	2539	2539	2539	2539	2539	2538	2539	2539
113	1795	1795	1795	1795	1795	1795	1794	1794	1794	1795	1795	1795	1795	1795	1793	1795	1794
114	1879	1879	1879	1879	1879	1879	1879	1878	1879	1879	1879	1872	1879	1879	1878	1879	1879
115	1953	1953	1953	1953	1953	1953	1953	1953	1953	1953	1953	1952	1953	1953	1952	1953	1952
116	2412	2412	2412	2412	2412	2412	2412	2412	2412	2412	2412	2412	2412	2412	2411	2412	2410
117	1535	1535	1535	1535	1535	1535	1535	1535	1535	1535	1535	1535	1535	1535	1534	1535	1535
118	2278	2278	2278	2278	2278	2278	2278	2278	2277	2278	2278	2278	2278	2288	2277	2278	2278
119	1987	1987	1987	1987	1987	1987	1987	1987	1987	1987	1987	1987	1987	1987	1986	1987	1987

Table 4. The beat annotation for the reviewed methods

[48]

[45]

[46]

Rec [5-24] [25] [26-30] [31] [32] [33] [34] [35] [36] [37-39] [40-42] [43] [44]

1518 1518

1619 1619

1963 1963

2136 2136

2980 2980

2656 2656

1860 1860

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				Table	4. The	beat a	nnotat	ion fo	r the r	eviewe	d metl	ods (c	ontinu	e)			
Rec	[5-24]	[25]	[26-30]	[31]	[32]	[33]	[34]	[35]	[36]	[37-39]	[40-42]	[43]	[44]	[45]	[46]	[47]	[48]
208 209	2955	2955 3005	2955	2955 3004	2955	2955	2955	2955	2955	2955	2955 3004	2955	2955	2946 3005	2954	2955	2921
210	3005 2650	2650	3005 2650	2650	3005 2650	3004 2650	3005 2650	3004 2650	3004 2650	3004 2650	2650	3004 2650	3004 2650	2647	3004 2649	3005 2650	3002 2644
212	2748	2748	2748	2748	2748	2748	2748	2748	2748	2748	2748	2748	2748	2748	2747	2748	2747
213	3251	3251	3251	3251	3251	3251	3250	3250	3250	3251	3251	3251	3251	3251	3249	3251	3249
214	2262	2262	2262	2261	2261	2261	2262	2261	2261	2265	2265	2265	2265	2254	2261	2262	2261
215 217	3363 2208	3363 2208	3363 2208	3363 2208	3363 2208	3361 2208	3363 2208	3363 2208	3363 2208	3363 2209	3363 2209	3363 2209	3363 2209	3353 2208	3362 2207	3363 2208	3362 2208
217	2154	2154	2154	2154	2154	2154	2154	2154	2154	2154	2154	2154	2154	2154	2153	2154	2154
220	2048	2048	2048	2048	2048	2048	2047	2048	2047	2048	2048	2048	2048	2048	2047	2048	2047
221	2427	2427	2427	2427	2427	2427	2427	2427	2426	2427	2427	2427	2407	2427	2426	2427	2427
222	2483	2483	2483	2483	2483	2483	2483	2483	2483	2483	2483	2483	2483	2484	2482	2483	2482
223 228	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2053	2605 2048	2605 2053	2605 2053	2604 2052	2605 2053	2603 2053
230	2256	2256	2256	2256	2256	2256	2256	2256	2256	2256	2256	2256	2256	2256	2255	2256	2256
231	1571	1571	1571	1571	1571	1571	1571	1571	1571	1571	1571	1571	1571	1571	1570	1571	1571
232	1780	1780	1780	1780	1780	1779	1780	1780	1780	1780	1780	1780	1780	1780	1779	1780	1780
233	3079	3079	3079	3079	3079	3079	3079	3079	3078	3079	3079	3079	3079	3079	3078	3079	3071
234 T	2753 109494	2753 109493	2753 109496	2753 109492	2753 109495	2753 109488	2753 109488	2753 109486	2753 109481	2753 109508	2753 109510	2753 109483	2753 109488	2753 109478	2752 109443	2753 109428	2753 109328
Ē	0	1	2	2	3	6	6	8	13	16	18	23	36	44	51	66	166
Rec	[49]	[50]	[51-56]	[57]	[58]	[59]	[60]	[61-63]	[64]	[65]	[66]	[67]	[68]	[69]	[70]	[71]	[72]
100	2269	2273	2273	2273	2267	2265	2273	2273	2273	2273	2273	2273	2274	2270	2273	2273	2272
101	1862	1864	1865	1865	1859	1860	1865	1865	1865	1865	1865	1865	1866	1862	1865	1873	1864
102 103	2183 2081	2187 2084	2187 2084	2187 2084	2181 2081	2180 2078	2187 2084	2187 2084	2187 2084	2187 2084	2187 2084	2187 2084	2187 2084	2186 2083	2187 2084	2186 2084	2186 2083
103	2225	2226	2230	2230	2224	2222	2230	2229	2229	2230	2229	2229	2229	2219	2229	2235	2228
105	2582	2566	2572	2572	2564	2565	2572	2572	2572	2572	2572	2572	2602	2559	2572	2578	2571
106	2024	2023	2027	2027	2024	2021	2027	2027	2027	2027	2027	2027	2026	2025	2027	2096	2026
107 108	2133 1761	2135 1759	2137 1763	2137 1763	2131 1757	2131 1757	2137 1763	2137 1763	2137 1763	2137 1763	2137 1763	2137 1763	2136 1763	2135 1747	2137 1774	2138 1763	2136 1762
108	2528	2527	2532	2532	2526	2524	2532	2532	2532	2532	2532	2532	2533	2531	2532	2519	1649
111	2121	2123	2124	2124	2120	2118	2124	2124	2124	2124	2124	2124	2123	2120	2124	2124	2123
112	2535	2539	2539	2539	2536	2531	2539	2539	2539	2539	2539	2539	2539	2537	2539	2549	2538
113	1791	1795	1795	1797	1791	1789	1795	1795	1795	1795	1795	1795	1794	1792	1795	1795	1794
114 115	1875 1949	1832 1953	1879 1953	1879 1953	1872 1945	1872 1946	1879 1953	1879 1953	1879 1953	1879 1953	1879 1953	1879 1953	1890 1953	1878 1950	1879 1953	1885 1960	1878 1952
116	2408	2392	2412	2412	2409	2404	2412	2412	2412	2412	2412	2412	2395	2407	2412	2401	2411
117	1532	1535	1535	1535	1532	1530	1535	1535	1535	1535	1535	1535	1535	1534	1535	1538	1534
118	2275	2278	2275	2275	2273	2271	2275	2278	2278	2278	2278	2278	2278	2275	2288	2298	2277
119	1984	1987	1987	1987	1985	1981	1987	1987	1987	1987	1987	1987	1988	1985	1987	2010	1986
121 122	1859 2472	1863 2476	1863 2476	1863 2476	1858 2471	1856 2468	1863 2476	1863 2476	1863 2476	1863 2476	1863 2476	1863 2476	1863 2476	1860 2475	1863 2476	1871 2477	1862 2475
123	1515	1518	1518	1518	1514	1513	1518	1518	1518	1518	1518	1518	1519	1517	1518	1518	1517
124	1616	1619	1619	1619	1613	1613	1619	1619	1619	1618	1619	1619	1619	1618	1619	1602	1618
200	2597	2600	2601	2601	2595	2593	2607	2601	2601	2601	2601	2601	2601	2560	2601	2599	2600
201 202	1961 2132	1934 2132	1963 2136	1963 2136	1946 2134	1959 2128	1963 2136	1963 2136	1963 2136	1963 2136	1963 2136	1963 2136	1949 2138	1954 2134	2000 2136	1963 2135	1962 2135
203	3003	2926	2982	2978	2976	2973	2982	2980	2980	2980	2980	2980	2988	2962	2980	2982	2979
205	2652	2653	2656	2656	2650	2648	2656	2656	2656	2656	2656	2656	2656	2654	2656	2657	2655
	1855	1857	1862	1862	1856	1850	1862	2332	2332	2332	2332	1543	2324	2246	2332	1862	2331
208 209	2951 3001	2940 3005	2956 3004	2954 3004	2953 2999	2946 2997	2956 3004	2955 3005	2955 3004	2955 3005	2955 3005	2955 3006	2953 3006	2937 3002	2955 3005	2952 3051	2954 3004
210	2646	2628	3004 2647	2647	2645	2642	2647	2650	2650	2650	2650	2640	2652	2640	2650	2645	2649
212	2744	2748	2748	2748	2746	2740	2748	2748	2748	2748	2748	2748	2748	2746	2748	2761	2747
213	3246	3250	3251	3251	3245	3241	3251	3251	3251	3251	3251	3471	3250	3247	3251	3245	3250
214		2258	2262	2262	2255	2254	2262	2262	2262	2262	2262	2259	2262	2259	2262	2273	2261
215	3358 2205	3363 2207	3363 2208	3362 2208	3357 2202	3353 2202	3363 2208	3363 2208	3363 2208	3363 2208	3363 2208	3363 2208	3362 2208	3360 2207	3363 2208	3398 2270	3362 2207
219	2151	2154	2154	2154	2150	2147	2154	2154	2154	2154	2154	2154	2154	2152	2287	2154	2153
220	2044	2047	2048	2048	2041	2041	2048	2048	2048	2048	2048	2048	2048	2047	2048	2068	2047
221	2423	2426	2427	2427	2422	2420	2427	2427	2427	2427	2457	2427	2427	2426	2427	2447	2426
222 223	2478 2601	2481 2604	2484 2605	2484 2605	2492 2603	2474 2581	2484 2605	2483 2605	2483 2605	2483 2605	2483 2605	2483 2589	2485 2604	2481 2604	2483 2605	2624 2636	2482 2604
228	2050	2050	2053	2003	2048	2047	2003	2053	2053	2053	2053	2053	2060	2051	2003	2116	2052
230		2256	2256	2256	2252	2248	2256	2256	2256	2256	2256	2256	2256	2253	2256	2257	2255
231	1568	1571	1886	1886	1566	1565	1186	1571	1571	1571	1571	1571	1571	1570	1573	1569	1570
232	1778	1780	1780	1767	1719	1776	1780	1780	1780	1780	1780	1780	1783	1779	1780	1734	1779
233 234	3074 2749	3078 2753	3079 2753	3076 2753	3135 2747	3069 2745	3079 2735	3079 2753	3079 2753	3079 2753	3079 2753	3079 2753	3077 2751	3076 2751	3079 2753	3074 2763	3078 2752
		109255		109788		109134					109996	109369		109663			
E	203	239	329	348	357	360	423	472	473	474	502	567	579	603	665	738	1400

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