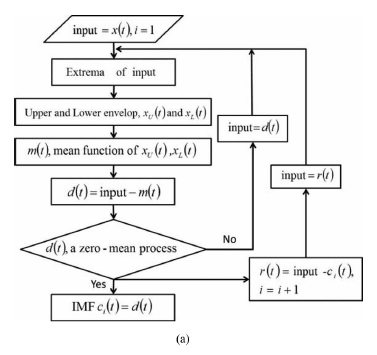
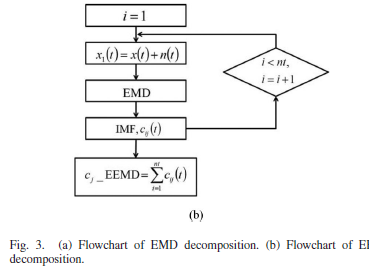
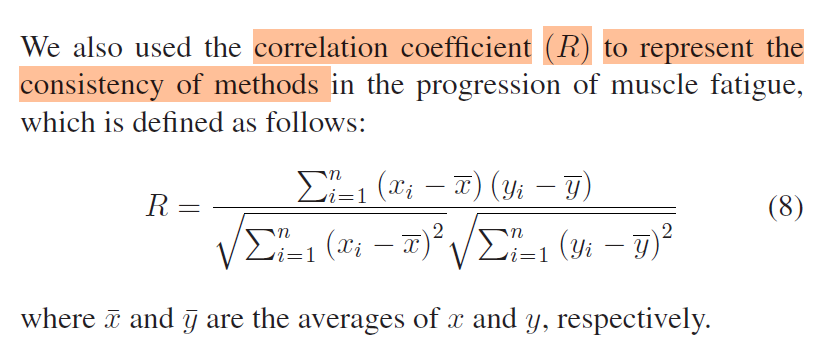
It is well known that the power spectrum of the sEMG shifts to a lower frequency during a sustained muscle contraction. The spectral parameters, such as the mean frequency (MNF) and the median frequency (MF), are the manifestation of localized muscle fatigue.

The Progression of Muscle Fatigue During Exercise Estimation With the Aid of High-Frequency Component Parameters Derived From Ensemble Empirical Mode Decomposition

A useful nonstationary and nonlinear signal processing technique, known as empirical mode decomposition (EMD), has been proposed. With an iterative decomposition of signals, EMD separates the full signal into ordered elements with frequencies ranging from high to low in each intrinsic mode function (IMF) level. Results showed that HHT-derived (Hilbert-Huang Transform) spectral and linear regression parameters were consistent and more reliable than those obtained with the short-time Fourier transform and the wavelet transform.

The procedure of the Ensemble EMD is to add statistically zero-mean noise into the signal with sufficient trials, and the ensemble IMF is estimated by the summation of the IMF from each trial of the same level. The goal of this study is not to quantify the myoelectric manifestation of muscle fatigue. Our goal is to find a more sensitive and stable method to sense the progression of muscle fatigue in the local muscle during exercise.





Proposed Fatigue Index for the Objective Detection of Muscle Fatigue Using Surface Electromyography and a Double-Step Binary Classifier

They suggested that the frequency spectrum of the EMG can be classified into three regions, namely,

* low-frequency components (LFC) (20–45 Hz),
* intermediate-frequency components (IFC) (46–80 Hz),
* high-frequency components (HFC) (81–350 Hz).

It is suggested that the power of the LFC increases, while that of the HFC decreases.

Fatigue occurs when the power of the LFC is equal to the power of the HFC (<https://ieeexplore.ieee.org/document/7591924/>).

The segmented EMG signal was filtered by two band-pass filters separately to produce two sub-signals, namely,

* a high-frequency sub-signal (HFSS) and
* a low-frequency sub-signal (LFSS).

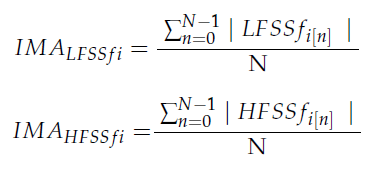
Then, the instantaneous mean amplitude (IMA) was calculated for the two sub-signals to ultimately obtain the fatigue index, which represents

the difference between the IMA values of the LFSS and HFSS, respectively.

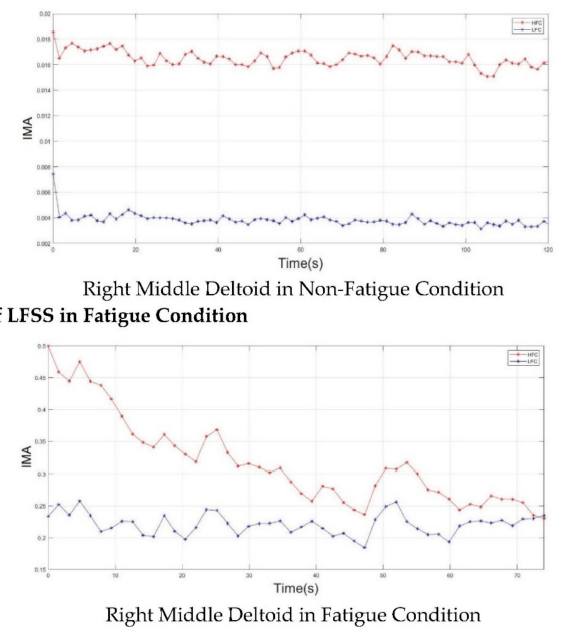
* The high-frequency components had been identified to be in the range of 80–350 Hz.
* The LFC lay in the range of 25–79 Hz.

An kai erxetai se antithesi me theoria einai afto pou ulopoieitai sto paper. Apofevgetai h xrhsh tou intermediate component.

Then, the fast Fourier transform (FFT) was applied to these sub-signals to produce the LFSSf and HFSSf.



Apo katw einai ta duo IMA gia to LFC kai to HFC. Apo oti fainetai se afton h otan to low perasei to high exoume fatigue. Afto genika to akolouthisa sthn diplwmatiki alla se emena ta IMA den suberiferontai etsi. Pistevw pws paizei polu rolo to oti einai allos mus giati aftos exei kanei sto xeri thn askhsh.



For an accurate evaluation and in considering each sEMG signal as having segments of length N, the fatigue indices of the first and last three sEMG segments of all the subjects in fatigue condition were calculated. A fatigue index with a negative value was an indication of non-fatigue, while a zero or positive value was an indication of fatigue.

HIGH ACCURACY RECOGNITION OF MUSCLE FATIGUE BASED ON SEMG MULTIFRACTAL AND LSTM

more research into changes in the local features of various levels of sEMG signals is necessary using the multifractal technology. A spectrum that depicts a subset and the appropriate fractal dimension is typically used to define multifractals. The major algorithms are:

* multifractal detrended fluctuation analysis (MFDFA)
* multifractal detrended moving average (MFDMA).

According to the calculations that MFDMA can perform , the four multiple fractal characteristics of SOM, DOM, DFS and PSE widths of the multifractal spectra were wider during fatigue than when they were during non-fatigue.

The multifractal spectra are symmetrical along the approximate axis in the non-fatigued condition, but with muscular fatigue, this symmetry tendency is greatly diminished.

The SOM, DOM and PSE features have clear feature distinctions between the non-fatigue and fatigue states, and the feature overlap rate of the two states is low,

whereas the DFS features have a greater overlap, and the distinction is less clear.

The difference between the aforementioned mean values of the properties of the myoelectric signals of 10 subjects under the fatigue and non-fatigue scenarios was observed using the t-test method in order to further determine whether the SOM, DOM, DFS and PSE extracted by the MFDMA algorithm have statistically significant differences under such scenarios.

According to the findings, the three characteristics (SOM, DOM and PSE) that were derived from the multiple fractal spectrum using the MFDMA method were statistically significant (P-value 0.01) in determining whether or not the muscles were exhausted.

Comparatively, the difference in DFS variability is relatively small. The findings could offer a fresh feature reference for deep learning and machine learning models that recognize muscle fatigue.