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### 1. Overview

Retrospective is a software utility and graphical user interface to reconstruct self-gated cardiac or respiratory CINE MRI acquired with an MR Solutions preclinical MRI system.

Reconstruction is based on compressed-sensing after retrospective sorting of the data into cardiac and/or respiratory time frames, using a navigator signal for cardiac and respiratory synchronization.

### 2. Contact

Retrospective and this manual is written by:

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#### 3. Disclaimer

The software has been extensively tested using mouse data acquired with an MR Solutions preclinical 7.0T/24cm system.

However, this does not warrant the functions contained in the program will meet your requirements or that the operation of the program will be uninterrupted or error-free.

In case of questions or issues, please contact Gustav Strijkers.



### 4. Installation notes

#### Software download

Matlab source code and a Windows standalone version (using the free Matlab runtime engine) can be downloaded from github:

https://github.com/Moby1971?tab=repositories

#### Installation of the Windows standalone version

MyAppInstaller web.exe

Will install the Matlab runtime engine and the Retrospective program.

# **Bart toolbox download**

The advanced reconstruction options in Retrospective require the Bart reconstruction toolbox, which can be downloaded from:

https://mrirecon.github.io/bart/

### Bart toolbox installation in OSX

- (1) Install Xcode from the Mac App Store
- (2) Install MacPorts (http://www.macports.org/)
  It is recommended to install a newer version of gcc from MacPorts
- (3) Installation

```
$ xcode-select --install
$ sudo port install fftw-3-single
$ sudo port install gcc6 (or newer version)
$ sudo port install libpng
$ sudo port install openblas
$ make all clean
$ make
```



### **Bart toolbox installation in Windows 10**

(1) Install the Windows subsystem for Linux

Start a windows powershell and run the following command:

Enable-WindowsOptionalFeature -Online -FeatureName Microsoft-Windows-Subsystem-Linux

A system restart will be needed.

For more information, see:

https://docs.microsoft.com/en-us/windows/wsl/install-win10

(2) Download Ubuntu Linux 18.04

For more information see:

https://docs.microsoft.com/en-us/windows/wsl/install-manual

Install the appx file by double-clicking in Explorer or in a PowerShell command prompt:

Add-AppxPackage .\app\_name.appx

You will be asked to create a user account the first time you start a Linux command prompt.

- (3) Upgrade the Linux distribution
  - \$ sudo apt-get update
  - \$ sudo apt-get dist-upgrade
- (4) Install Bart prerequisites
  - \$ sudo apt-get install make gcc libfftw3-dev liblapacke-dev libpng-dev libopenblas-dev gfortran
- (5) Download Bart
  - \$ wget https://github.com/mrirecon/bart/archive/v0.4.02.tar.gz

For Windows Bart version 0.4.02 is recommended. Newer versions seem to compile but some functions which are required produce errors.

- (6) Build Bart
  - \$ tar xvfz v0.4.02.tar.gz
  - \$ cd bart-0.4.02
  - \$ make
  - \$ make utest
  - \$ make test
  - \$ sudo make PREFIX=/usr/local install



# 5. Running the software

# Running in Matlab 2020a

The Retrospective software can be started from its root directory from the command line.

```
>> retrospective
```

#### Notes:

(1) The Retrospective root directory ~/Retrospective contains the following 3 text files:

```
Bart toolbox installation directory
Delete this file if the Bart toolbox is not available on your system

dcmpath.txt
Shortcut to base directory in which the Dicom files will be stored

mrdpath.txt
Shortcut to base directory in which the MRI scanner-generated MRD files can be found

Make sure that the text files contain exactly 1 line of text
```

(2) Additional licenses may be required.

```
>> license('inuse')
communication_toolbox
distrib_computing_toolbox
image_toolbox
matlab
signal_blocks
signal toolbox
```

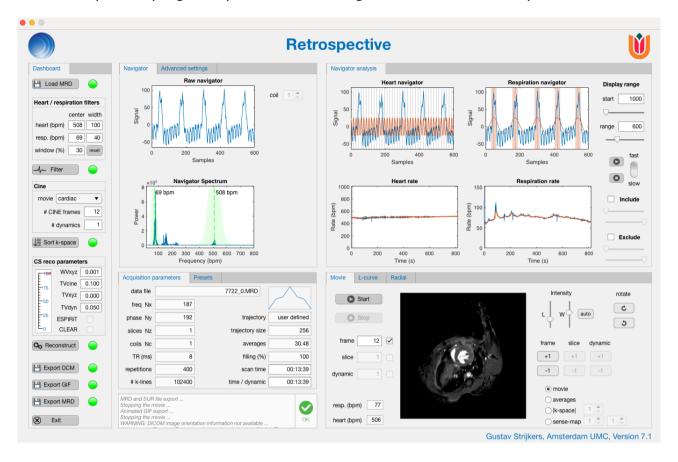
### **Running the Windows standalone**

The Windows standalone version can be run from the start menu or the desktop icon.



# 6. Basic operation

The Retrospective program operates from a single window with 5 main panels.



### Panel 1: Dashboard

This panel contains the task buttons that control the reconstruction process. The dashboard tasks need to be completed from top to bottom. A green light next to the task indicates that the task has been completed. When the light is yellow the task is busy. Red indicates not completed yet.

#### Panel 2: Acquisition parameters / Presets

This panel lists the relevant acquisition parameters and a few reconstruction presets.

### Panel 3: Navigator / Advanced settings

This panel shows the raw navigator signal, the navigator frequency spectrum, and some advanced navigator analysis parameters.

#### Panel 4: Navigator analysis

This panel shows the navigator signals filtered for cardiac and respiratory motion, as well as the heart and respiratory rates as function of time.

### Panel 5: Movie / L-curve / Radial

In this panel the reconstructed CINE movie is shown. There are advanced sub-panels for optimization of compressed-sensing reconstruction (L-curve analysis) and Radial reconstructions (work in progress).



# Step 1: Loading data

Press Load MRD to import load the MRD raw data file.

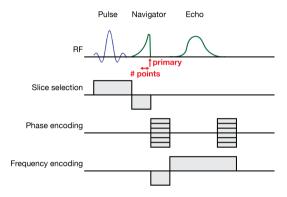
The data should include navigator data for cardiac and respiratory synchronization.

For data acquired with multiple receivers (phased-array RF coil) select 1 of the MRD files.

Relevant acquisition parameters will be shown in panel 2, including the k-space trajectory (linear, zigzag, or user defined).

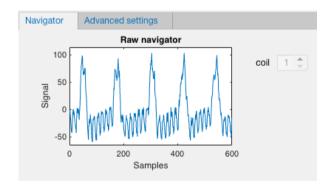
# Step 2: Inspecting the raw navigator signal

The in-slice navigator is generated by the refocusing properties of the slice selection gradient directly after the RF pulse, as shown in the figure below.



The raw navigator signal will contain rapid oscillations due to cardiac motion and slower

periodic peaks due to respiration.





For multi receiver coil data, individual navigators can be inspected with the **coil** toggle switch.

The respiration peaks in the navigator should be positive; in case they are negative, flip the signal with the **Flip** switch.

If cardiac and respiratory oscillations are not clearly visible, change the **primary** point slightly and increase **# points** (typically **# points** = 1 to 4) to see whether the quality improves.



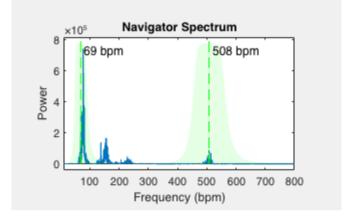
The panel also contains 2 presets for navigator filtering of mouse and rat data. These adapt the values **min/max heart** and **respiration rates**, which determine the search windows for the heart and respiration rate.

The parameter **freq Nx discard** determines the number of samples that are discarded between the end of the navigator and the beginning of the imaging echo. If an FID artifact is visible in the reconstructed images/movie, increase this number.

# Step 3: Inspecting the navigator power spectrum

The bottom part of panel 3 shows the power frequency spectrum of the raw navigator

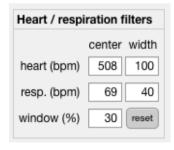
signal.



Typically, the spectrum looks as the figure above, with peaks (and higher harmonics) corresponding to the respiratory and cardiac frequencies. The program automatically determines the most likely respiratory and cardiac frequency.

Green shaded areas indicate the position and width of the Butterworth filters, which are used to filter the raw navigator and extract the periodic cardiac and respiratory motion as function of time.

In case the automatic respiration and/or cardiac frequency detection fails, the **center** and **width** filter values can be adjusted in the heart/respiration filters panel, shown below.



**Center** and **width** determine the center-frequency and width of the Butterworth filters for navigator filtering.

**Window (%)** determines the percentage of the data that is discarded during respiratory motion.

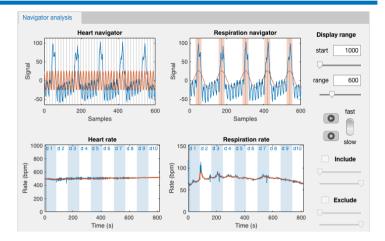
Press reset to reset the values.



# Step 4: Filter the navigator

Press Filter to filter the raw navigator signal and extract cardiac and respiratory motion as function of time.

The result may look like this:



The sliders can be used to change the display range to inspect the full data set.

Use buttons to automatically advance the navigator and inspect the data.

The top left figure shows in blue the raw navigator signal and in red the signal filtered for cardiac motion. The gray vertical lines indicate the peaks in the oscillations, which can be used to check the alignment between the red and blue signals.

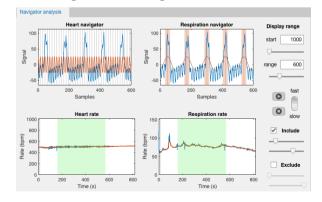
Bottom left is the resulting heart rate as function of during the full acquisition. The blue line is the heartbeat to heartbeat variation, whereas the red line is a smoothed trend-line.

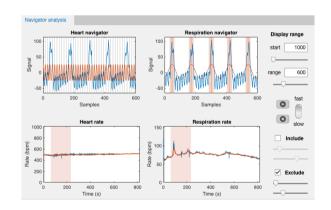
The top right figure shows in blue the raw navigator signal and in red the signal filtered for respiratory motion. The gray vertical lines indicate the peaks in the oscillations, which can be used to check the alignment between the red and blue signals. The shaded red areas indicates the part of the data which is discarded during respiratory motion.

Bottom right is the resulting respiration rate as function of during the full acquisition. The blue line is the respiration to respiration variation, the red line is a smoothed trend-line.

Heart and respiration rates should be smoothly varying over time. If this is not the case, adjust the Butterworth filter settings.

### Including / excluding data





In case of irregular respiration or heartbeat part of the data can be included (green) and/or excluded (red) by checking the **Include** or **Exclude** boxes or both. Including or excluding data is not possible for multi-slice 2D data.

After this, press \_\_\_ again to filter the data with the new settings.



## Step 5: Sort the k-space

Choose the desired sorting method, number of frames, and number of dynamics.

# **Sorting methods**

## (1) Cardiac

Cardiac phase-binning. Each heartbeat is divided into an equal number of cardiac CINE frames. The average time between cardiac frames is determined from the average heart-rate and the number of cardiac frames. This option is preferred for most applications, particularly for high frame-rate reconstructions for analysis of diastolic function.

Cine

movie cardiac

■ Sort k-space

# CINE frames

# dynamics

12

1

# (2) Cardiac abs.

Cardiac absolute-binning. A fixed frame time is predetermined from the average heart-rate and the number of cardiac CINE frames. This option could be more accurate for reconstruction of systolic function in the presence of heart-rate variations, but leads to temporal blurring in the diastolic phase.

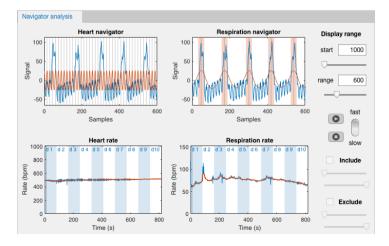
# (3) Respiratory

Respiratory phase-binning. Each respiration cycle is divided into an equal number of respiratory frames. The average time between respiratory frames is determined from the average respiration-rate and the number of desired respiration frames. When using this option, **window** (%) is neglected.

Press sort k-space to start sorting the data into k-space.

### **Dynamics**

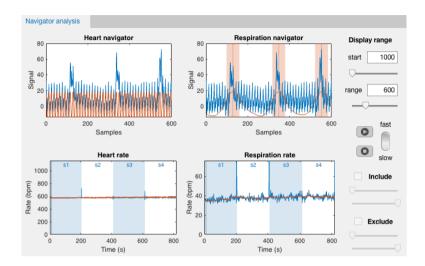
It is possible to reconstruct data in a dynamic time series, for example for dynamic-contrast enhanced acquisitions. Choose the desired number of dynamics, and continue with sorting k-space and reconstruction. The maximum number of dynamics is set to 600, but remember that k-space will become very sparse with high number of dynamics and reconstruction might take very long. The dynamic time-frames will be indicated in the heart rate and respiratory rate plots in blue/white shaded areas as shown below.





### Multi-slice 2D data

For multi-slice 2D acquisitions, the heart rate and respiration rate plots show when the subsequent slices were acquired with blue/white shaded areas. For multi-slice 2D data it is not possible to reconstruct different dynamics nor is it possible to include or exclude part of the scan.



### 3D data

Version 7.1 of Retrospective supports reconstructions of 3D data.



# Step 6: Reconstruction of the data

Before reconstruction, select the appropriate reconstruction settings and regularization parameters in the **CS reco** parameters panel.

Reconstruction is based on a compressed sensing algorithm with wavelet I1-norm regularization and total-variation regularization in spatial and time dimensions.

Some parameters are not available without the BART toolbox.



The **Presets** panel provides some pre-determined reconstruction settings for different applications

#### **Parameters**

# (1) WVxyz

Wavelet regularization parameter in the spatial (x, y, and z) dimensions. For the mouse cardiac CINE, a low (0.001) or zero value resulted in the best movie quality.

### (2) TVcine

Total variation constraint in the CINE dimension. Higher values lead to improved image quality but increased temporal smoothing. For the mouse CINEs, a value of 0.1 seems a good compromise between image quality and temporal smoothing.

### (3) **TVxyz**

Total variation constraint in the spatial dimension. Higher values smooth the movie in the spatial domain. For mouse CINEs, this parameter does not seem to improve image quality. Recommended value therefore is zero.

# (4) TVdyn

Total variation constraint in the dynamics dimension.

### For multi-coil data only

#### (5) **ESPIRIT**

ESPIRIT reconstruction (Magn Reson Med. 2014 Mar 71(3): 990–1001.). This includes GRAPPA and SENSE reconstruction.

### (6) CLEAR

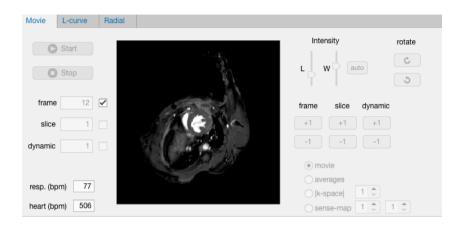
Intensity inhomogeneity correction using coil-sensitivity maps.

Press Reconstruct to start the reconstruction.



# Step 7: Viewing the movie

The resulting CINE MRI can be viewed in the Movie panel. Check the corresponding boxes to view the number of averages per k-line and cardiac frame, the k-space, or the coil sensitivity maps (ESPIRiT).



Press start to start the movie.

Press stop to stop the movie.

Check the corresponding boxes to loop the movie over frames, slices, and/or dynamics.

Image intensity can be adjusted with the level (L) and window (W) sliders.

Press or or to rotate the movie clockwise or counter clockwise (this will not affect the Dicom and MRD export orientations).

Press +1 or -1 below **frame** to advance or rewind the movie 1 time frame.

Different slices can be viewed with +1 or -1 below **slice**.

Advance dynamics with +1 or -1 below **dynamic**.

### Synchronizing different CINEs from one animal

Since the cardiac synchronization is not based on ECG triggering, CINEs from different slices or acquired in different orientations may not be synchronized with respect to each other, i.e. the end-systole and end-diastole might have different frame numbers.

To correct for this the following procedure can be followed. First stop the movie with the button. Then set the frame number to 1 in the dialog frame 1. Then, advance or rewind the movie with 1 or 1 to the desired starting phase of the cardiac cycle, for example end-diastole.

The cardiac synchronization will also be taken into account with DCM, GIF and MRD export.



# **Step 8: Movie export**

There are several ways to export the movies.



# (1) Export DCM

Exports the data in Dicom format for further processing in 3rd party software. The program searches for the Dicom information. If this information is not found, tags will be generated by the program itself. In the latter case the correct image position and orientation information are lost.

# (2) Export GIF

Generates animated-gif movie or movies (3D, multi-slice) of the reconstructed CINE. Image intensity (window, level) and image rotations are preserved.

# (3) Export MRD

The data will be stored as a new MRD data file in the same directory as the input MRD file. If the program finds an input rpr file, also a new rpr file will be generated. Additionally, when the program runs on the scanner computer, data will be reconstructed by the scanner software and new SUR files will be placed in the data directory for viewing and planning of next scans in the MR Solutions preclinical software.

Step 9: Exit

Press to shut down the program.