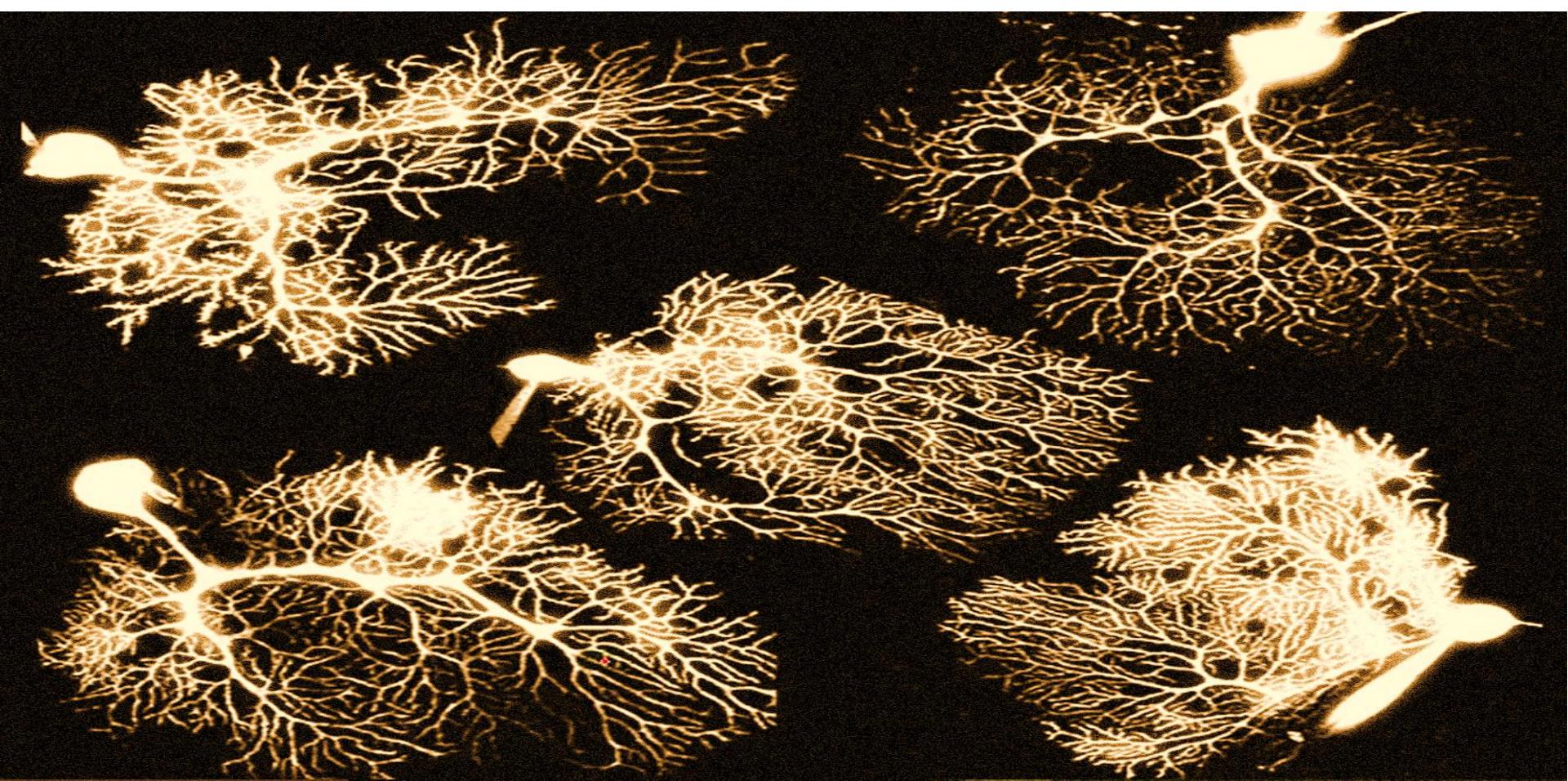


# Neuroscience of Learning, Memory, Cognition

## Part I: Neuronal Networks



1

Neuron Models

Set II

# Outline

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- Sensing & perception
- Neurons & spikes
- The Hodgkin-Huxley equation
- Modeling neuronal dynamics

Some slides credit:

- Adrienne Fairhall, Rajesh Rao, UW course material 2013-2017
- Wulfram Gerstner, EPFL course material 2018

Other credits as noted on slides

Cover slide drawing: Santiago Ramon Y Cajal

Textbooks:

- Peter Dayan & Larry Abbott “Theoretical Neuroscience”, 2005
- Wulfram Gerstner “Neuronal Dynamics”, 2014
- Eugene Izhikevich “Dynamical Systems in Neuroscience”, 2010

Reference book:

- Paul Miller “An Introductory Course in Computational Neuroscience”, 2018

# Outline

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- Sensing & perception
  - Neurons in the brain
  - Visual cortex & receptive fields
  - Vision & perception
- Neurons & spikes
  - Electrical personality of a neuron
  - Ionic channels
  - Action potential
- The Hodgkin-Huxley equation
  - The passive membrane
  - Voltage-gated channels
  - Anatomy of a spike
- Neuronal dynamics
  - Phase portrait models
  - Fixed points and their stability
  - Bifurcation (saddle-node / Hopf)
  - Simplified 2D models

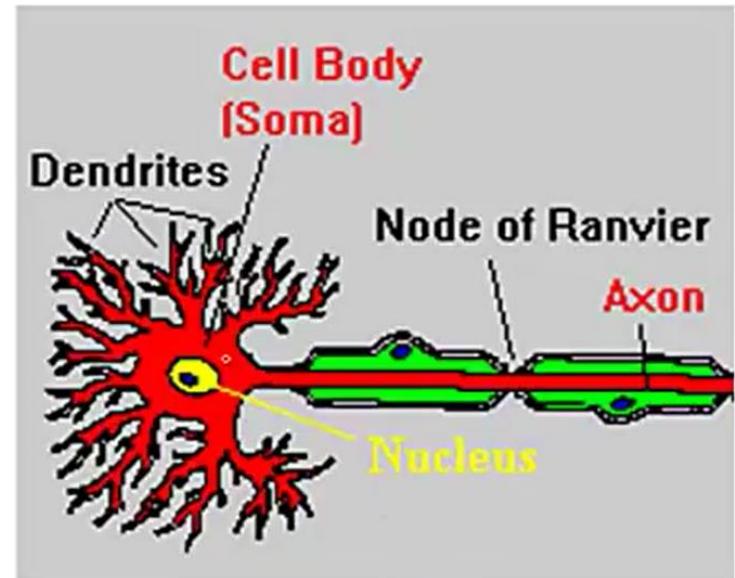
# Electrical Personality of a Neuron

neuron of a personality

# What is a Neuron?

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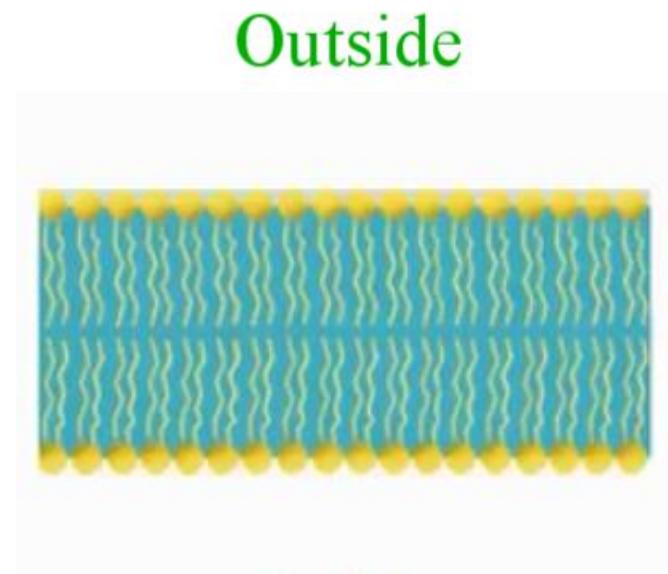
- A “leaky bag of charged liquid”
- Contents of the neuron enclosed within a *cell membrane*



# What is a Neuron?

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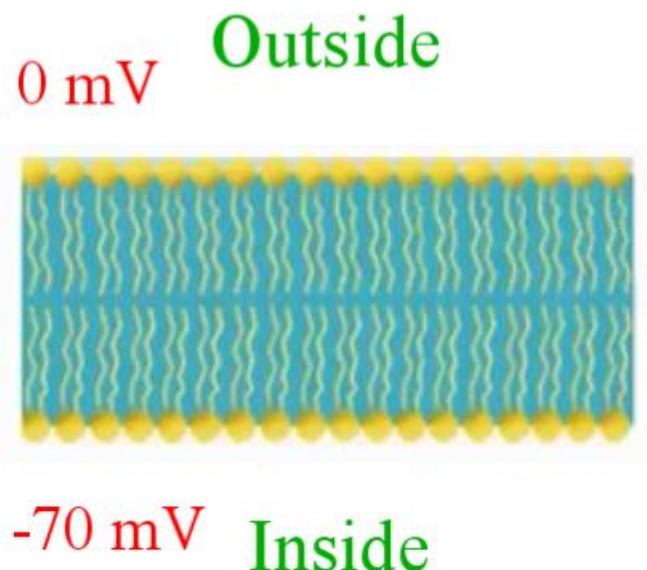
- A “leaky bag of charged liquid”
- Contents of the neuron enclosed within a *cell membrane*
- Cell membrane is a *lipid* bilayer
- Bilayer is **impermeable** to charged ion species such as  $\text{Na}^+$ ,  $\text{Cl}^-$ , and  $\text{K}^+$



# The Electrical Personality of a Neuron

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- Each neuron maintains a *potential difference* across its membrane  
→ Inside is about **-70 mV** relative to outside (*Resting Potential*)



# The Electrical Personality of a Neuron

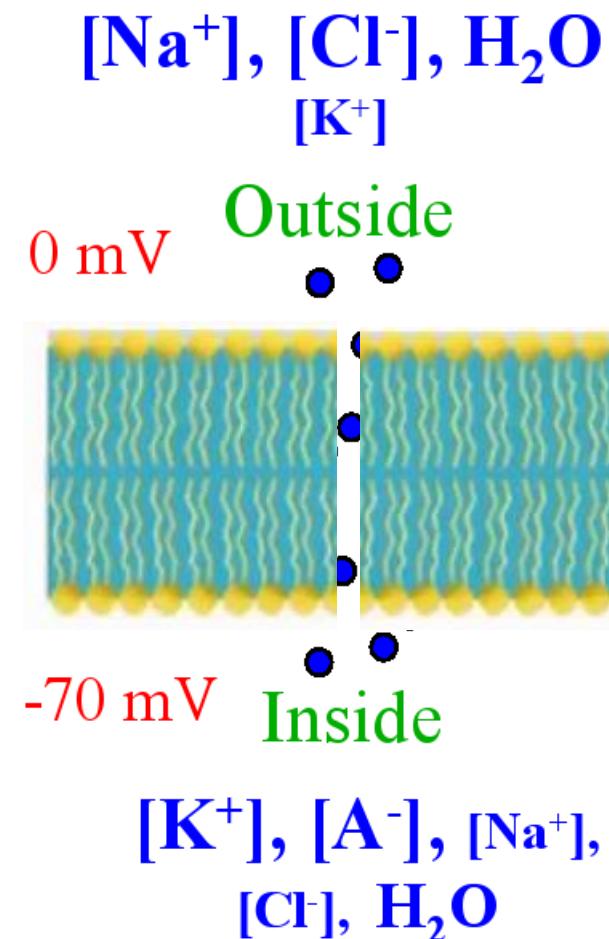
- Each neuron maintains a *potential difference* across its membrane  
→ Inside is about -70 mV relative to outside (*Resting Potential*)

$[Na^+]$  and  $[Cl^-]$  are higher outside;  
 $[K^+]$  and organic anions  $[A^-]$  are higher inside

(This causes **osmosis** forces)

*Ionic pump* maintains -70 mV difference by expelling  $[Na^+]$  out and allowing  $[K^+]$  ions in

(This is driven by **electric** forces)



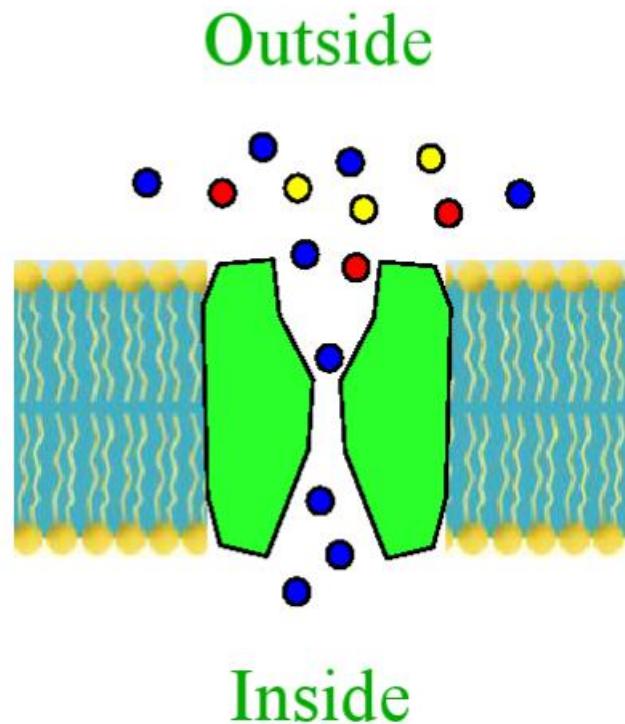
# Ionic Channels

ionic channels

# Ionic Channels: The Gatekeepers

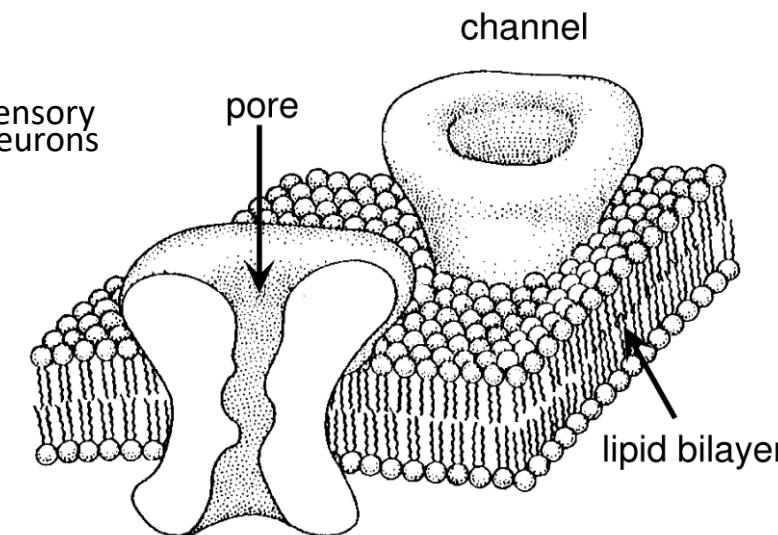
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- Ionic channels in membranes are proteins that are *selective* and allow only *specific ions* to pass through
  - E.g. Pass  $Na^+$  but not  $K^+$  or  $Cl^-$



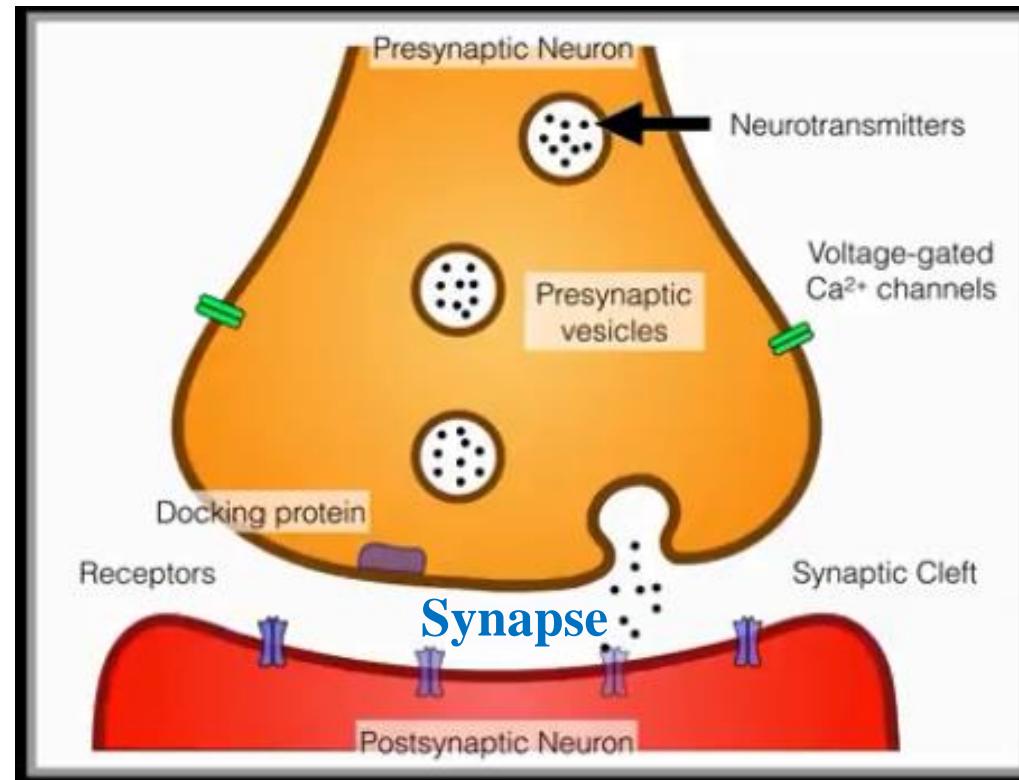
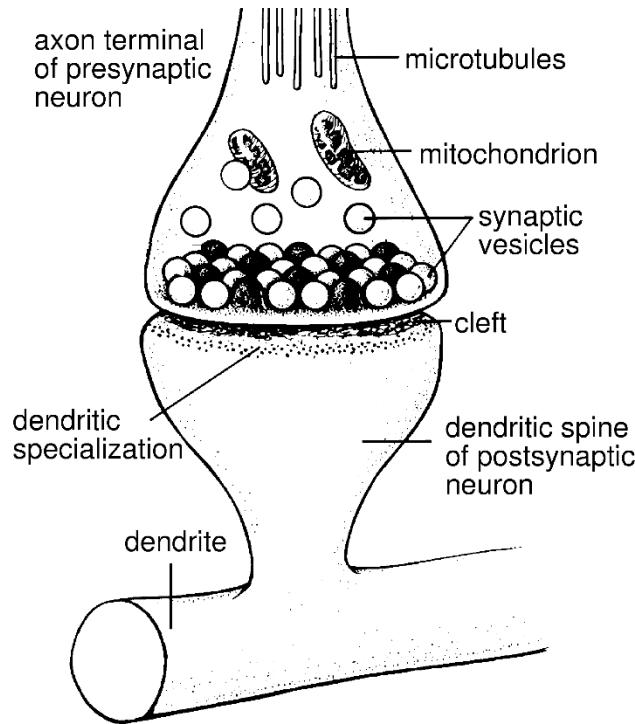
# Currents Flow through Ion Channels

- Ion channels distinguish between different ions  
→ Different ions have different rates of transport between inside and outside the neuron
- Ion channels are of many types:
  - Neurotransmitter-dependent (synaptic)
  - Voltage-dependent
  - Ca-dependent
  - Mechanosensitive
  - Heat sensitive



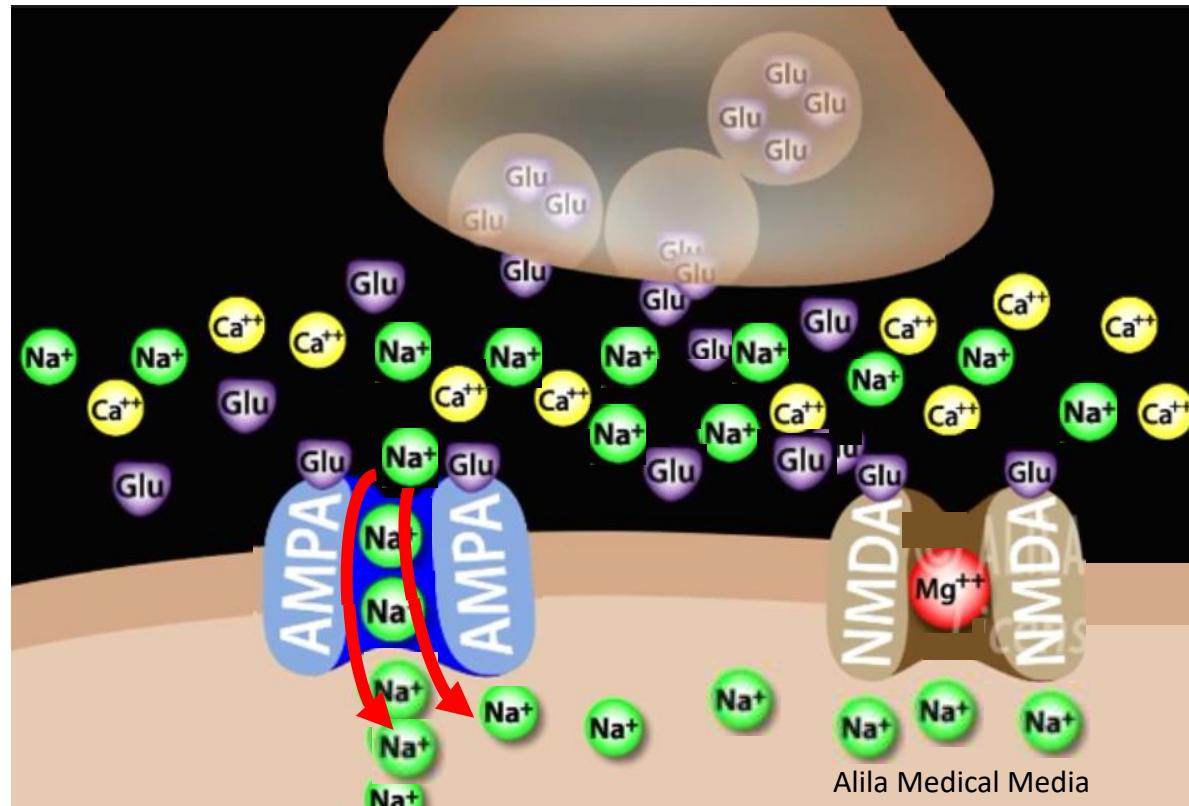
# Gated Channels Allow Neuronal Signaling

Inputs from other neurons → *Chemically-gated channels* (at *synapses*) open → Changes in local membrane potential



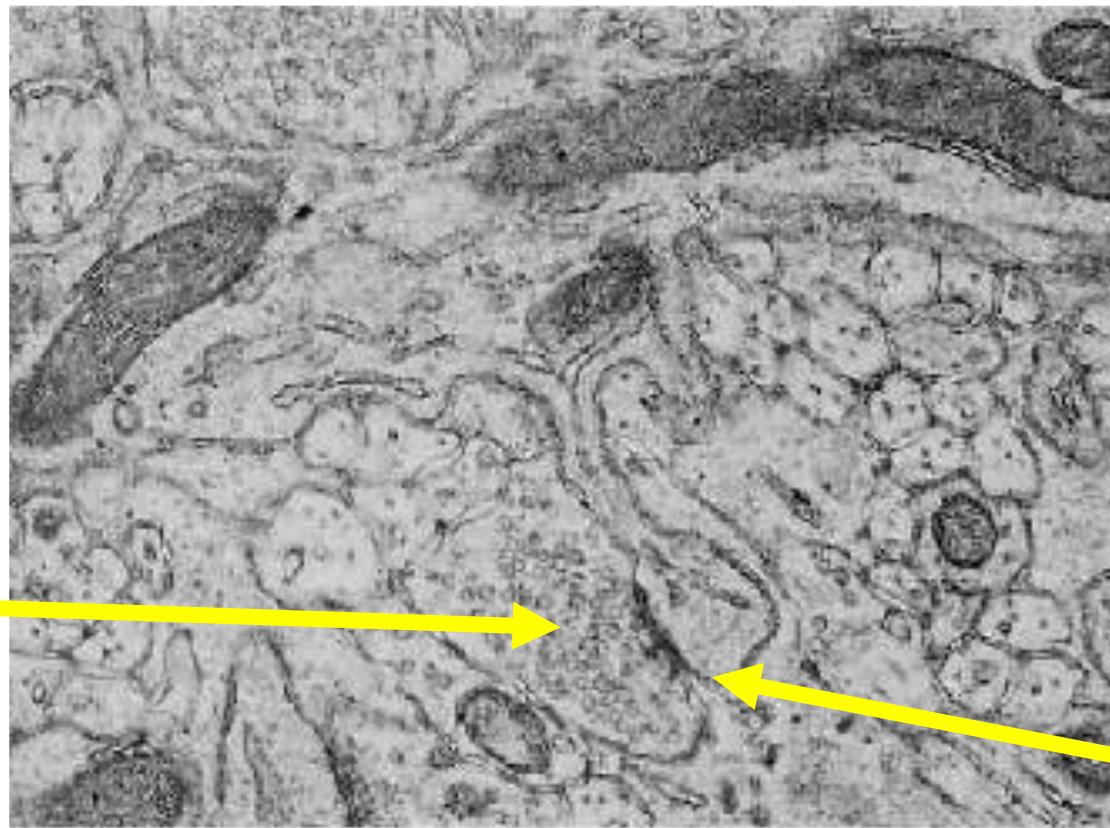
# Gated Channels Allow Neuronal Signaling

Inputs from other neurons → *Chemically-gated channels* (at *synapses*) open → Changes in local membrane potential



# How Synapses Work

Two membrane surfaces, of an axon and a dendrite, come together at a synapse: A 20 nm cleft separates them

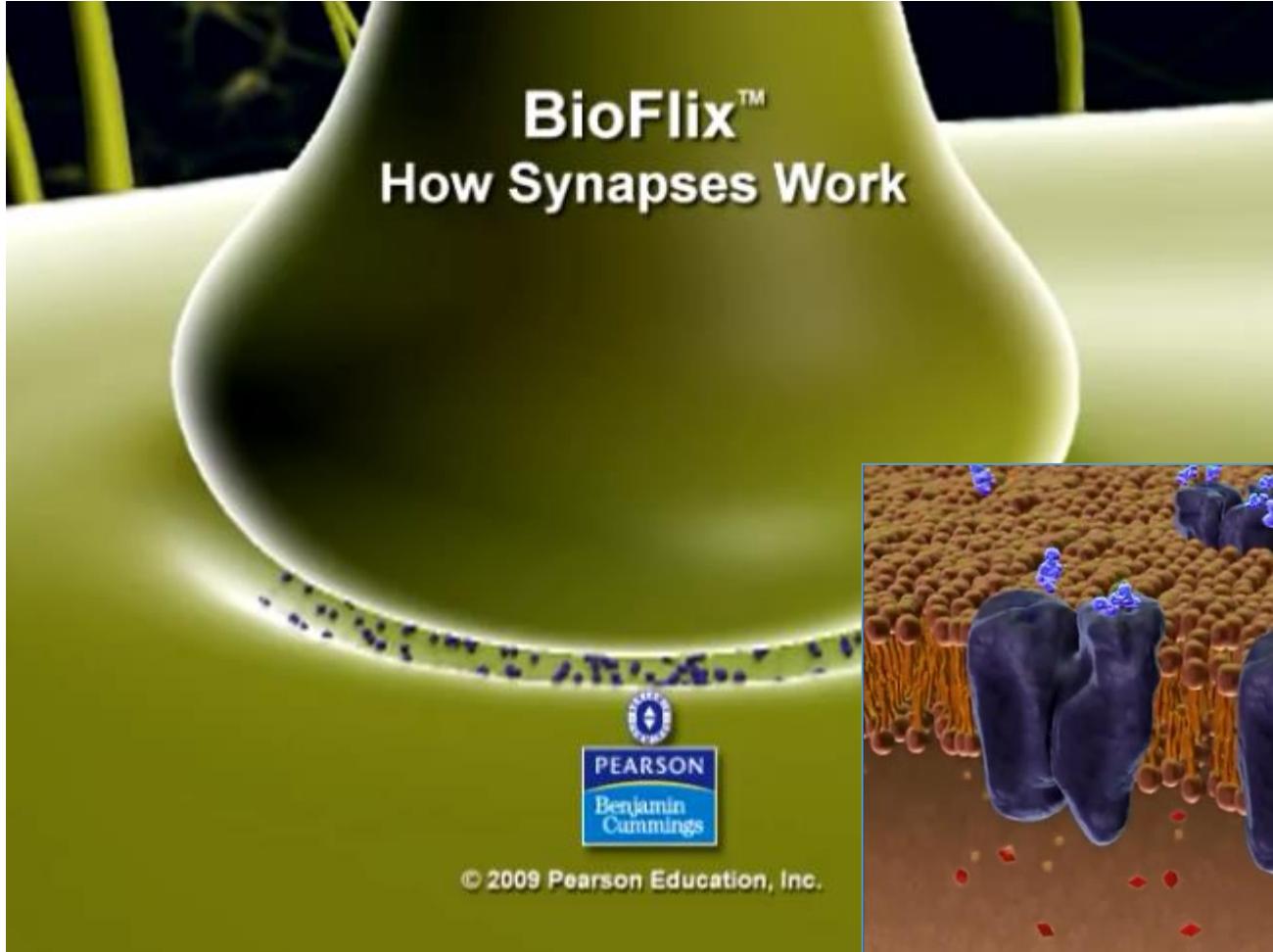


Electron microscope picture of a section through cerebellar cortex of a rat

A synapse

# How Synapses Work

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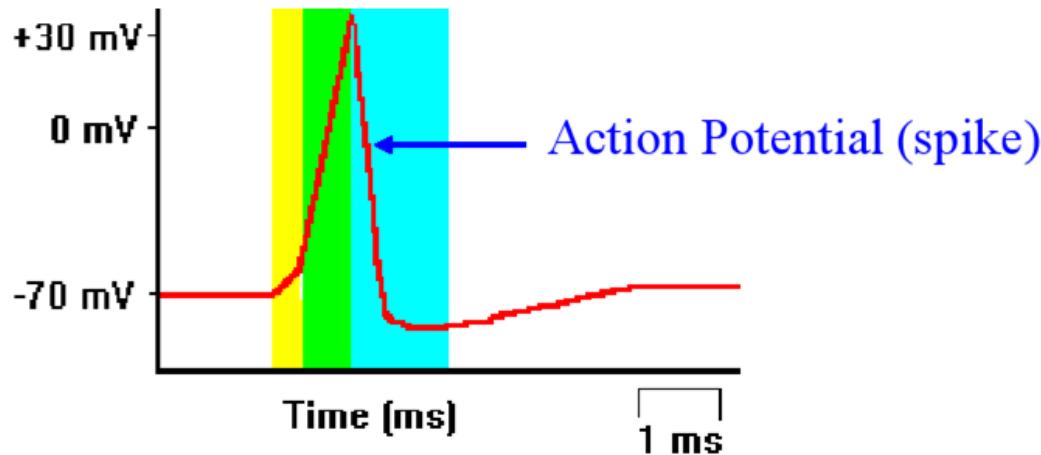
<https://www.youtube.com/watch?v=lbzfwtDtong>  
**(Video to watch later)**

# Action Potential

ACTION POTENTIAL

# The Output of a Neuron: Action Potential (Spike)

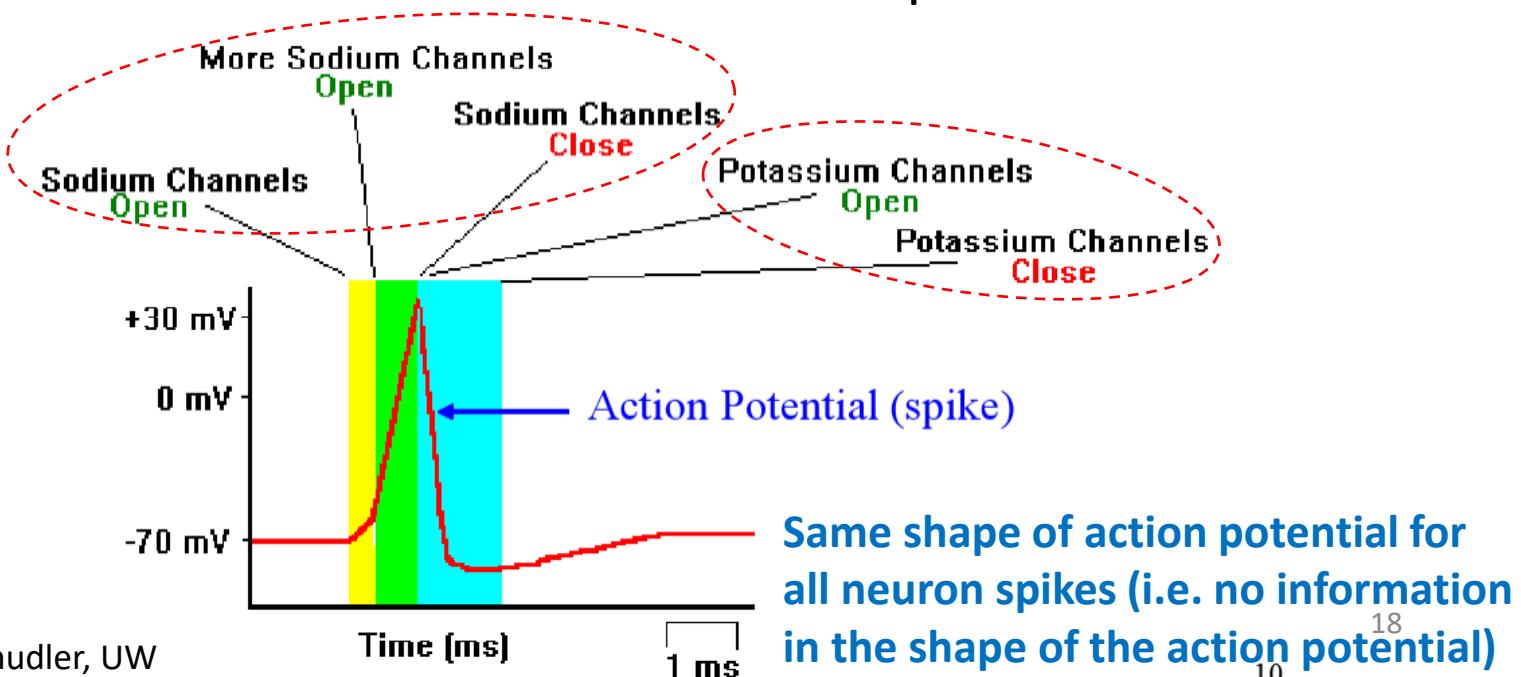
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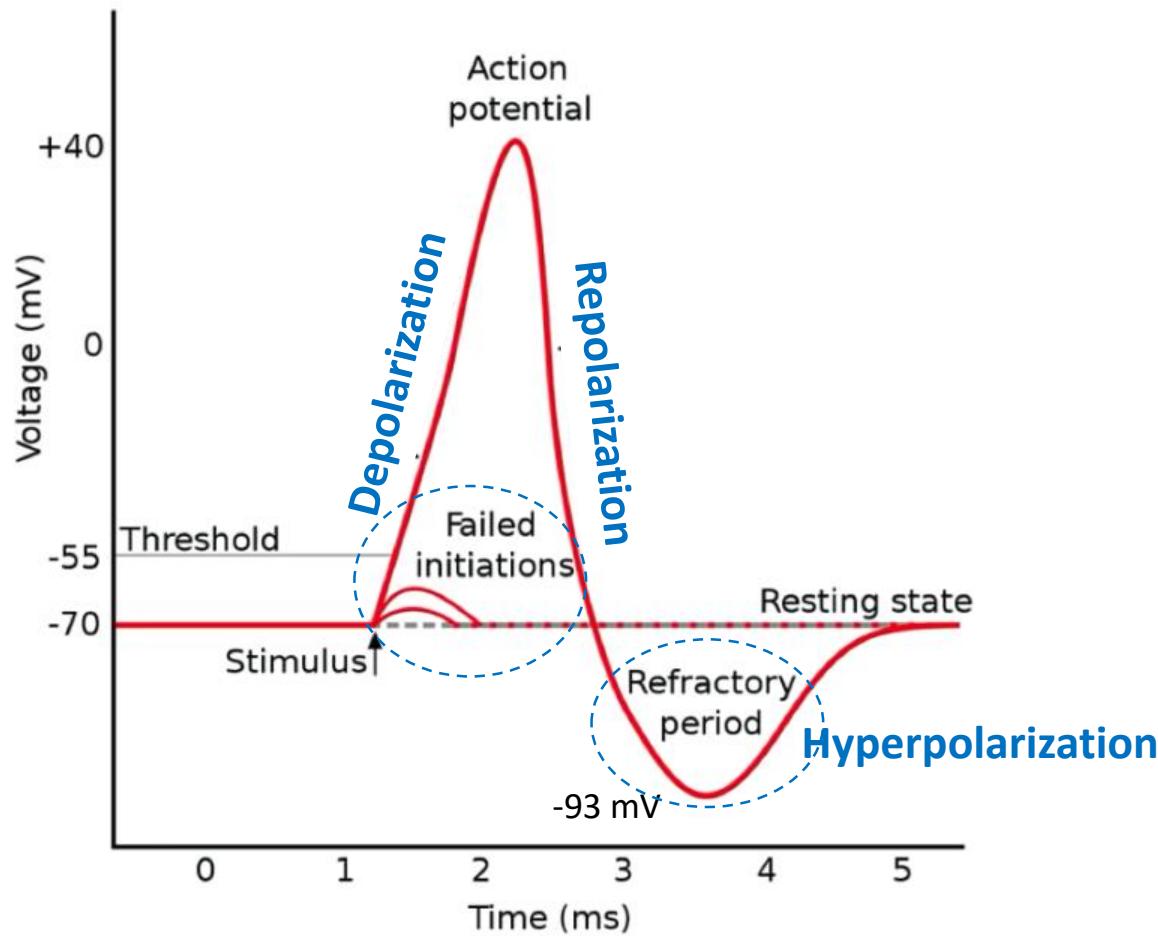
- Change of potential due to synaptic activity causes opening/closing of *voltage-gated channels* (in body, axon, dendrites)
  - Further *Depolarization* (positive change in voltage)
- Strong enough depolarization causes a spike or *action potential*

# The Output of a Neuron: Action Potential (Spike)

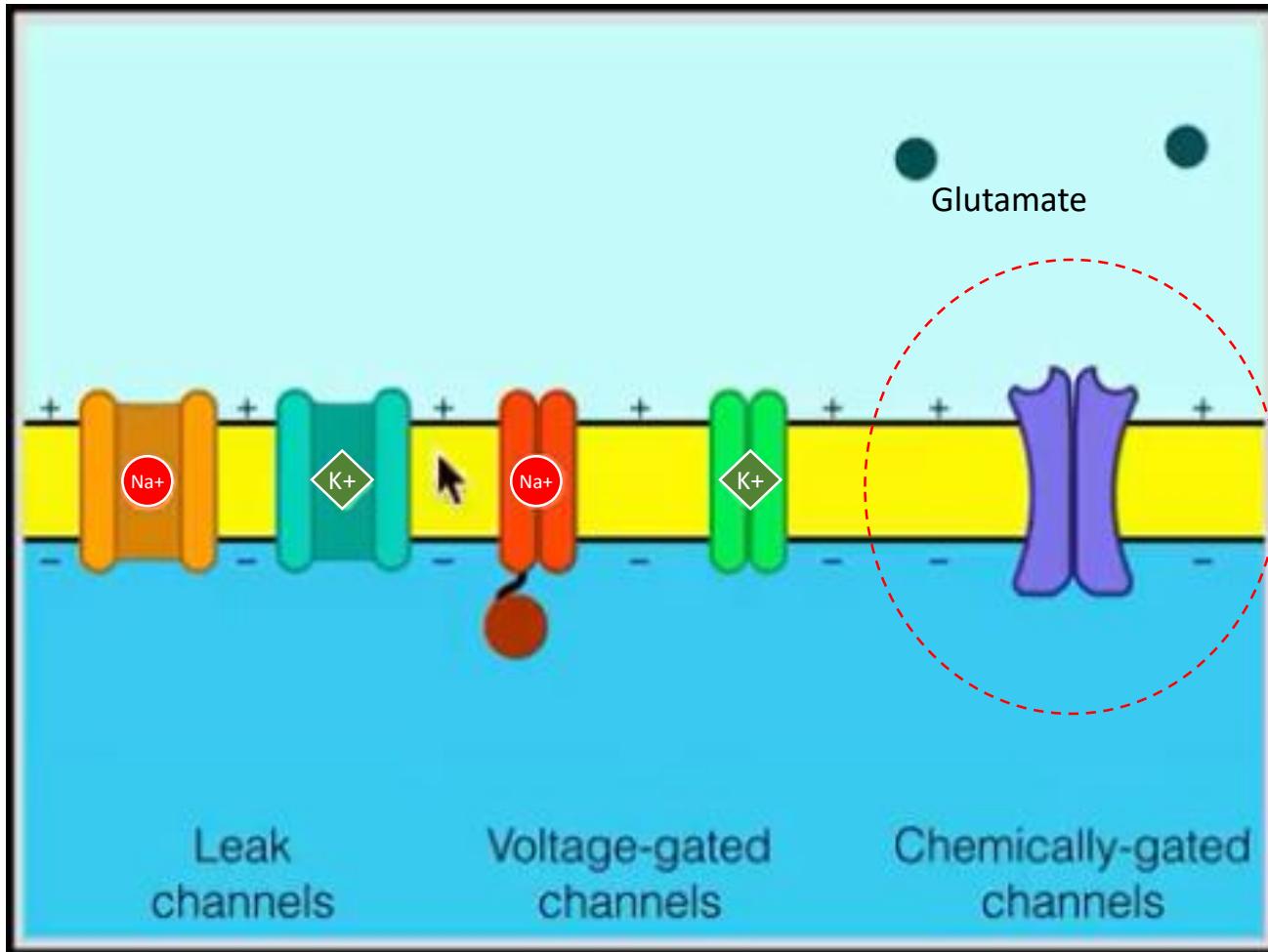
- *Voltage-gated channels* cause action potentials (spikes)
1. Strong *depolarization* opens  $Na^+$  channels, causing rapid  $Na^+$  influx and more channels to open (positive feedback)
  2. At higher potentials,  $Na^+$  channels inactivate while  $K^+$  *outflux* reduces and restores membrane potential



# The Output of a Neuron: Action Potential (Spike)



# Ionic Channels – Chemically-Gated Channels (Synapses)

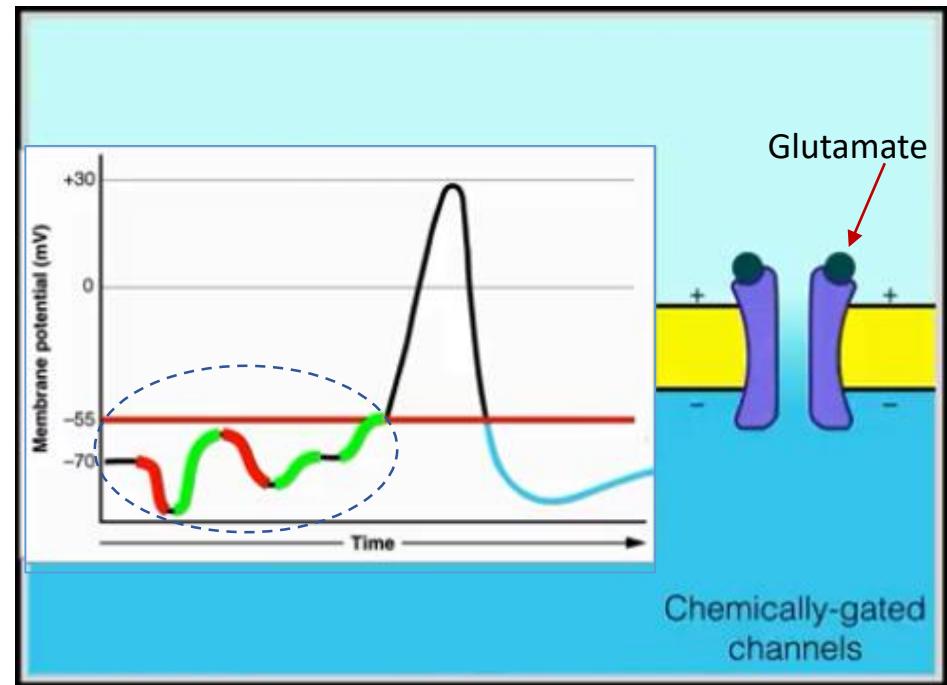


<https://www.youtube.com/watch?v=L41TYxYUqqs>  
*(Video to watch later)*

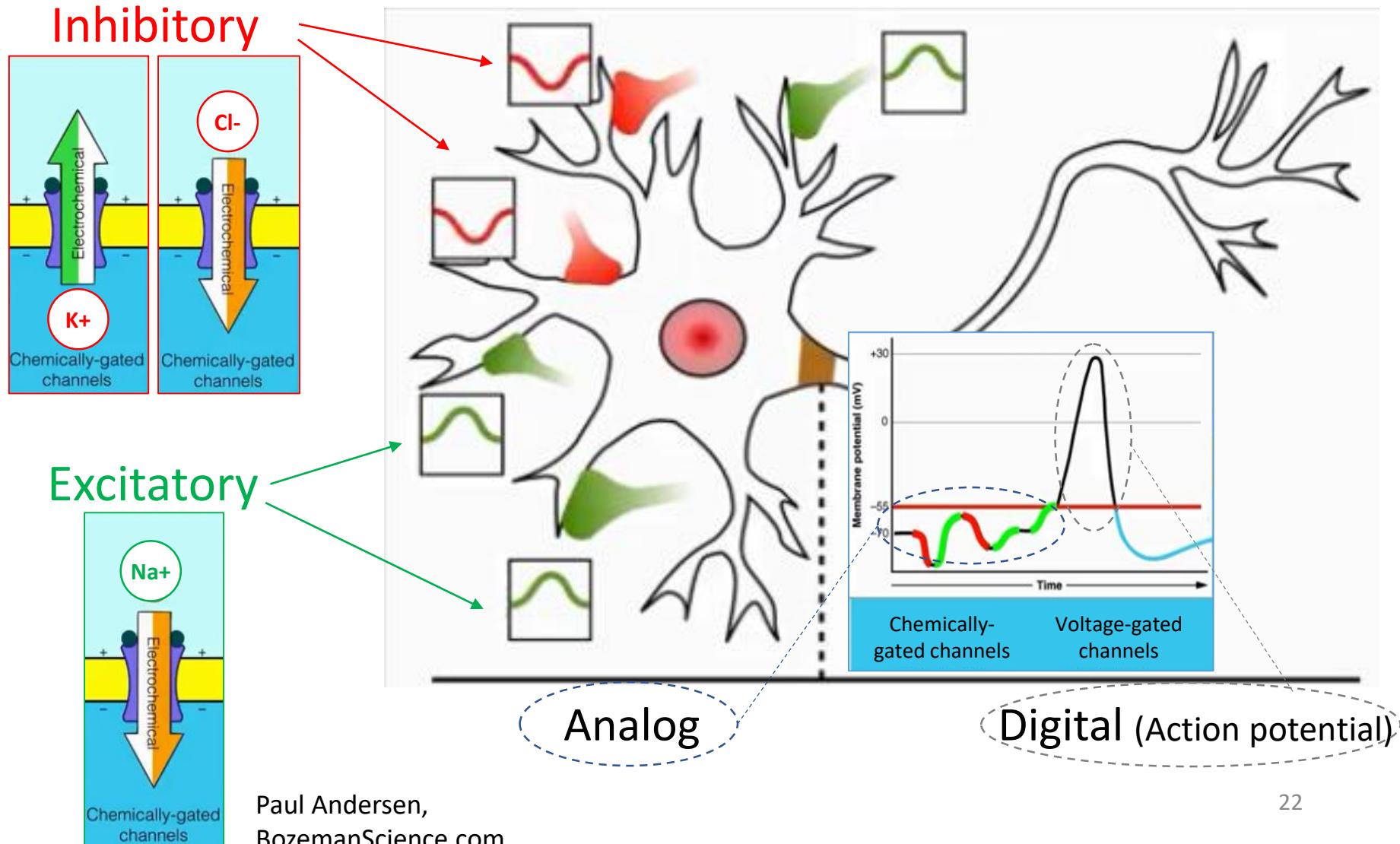
# Ionic Channels – Chemically-Gated Channels (Synapses)

Two types of chemically-gated channels:

- **Excitatory channels** tend to increase the membrane potential
- **Inhibitory channels** decrease the membrane potential

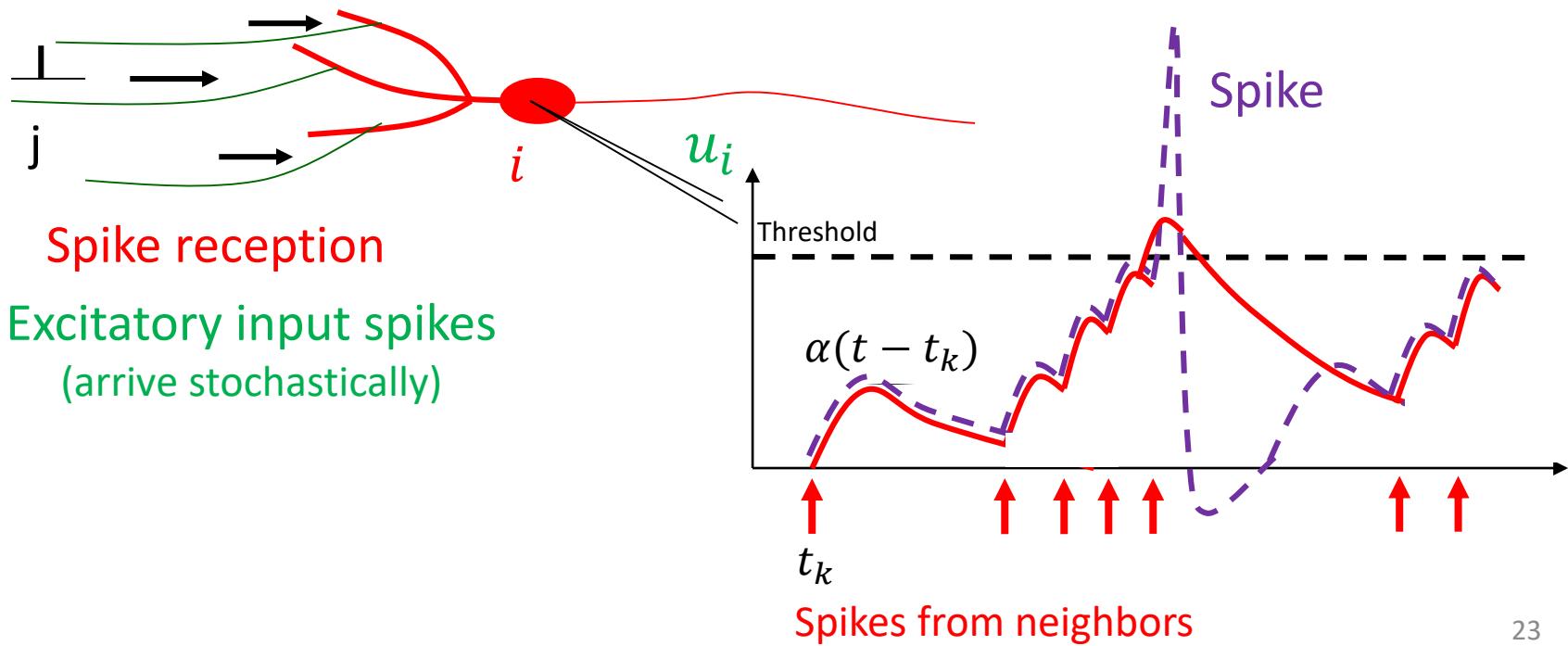


# Ionic Channels – Chemically-Gated Channels (Synapses)

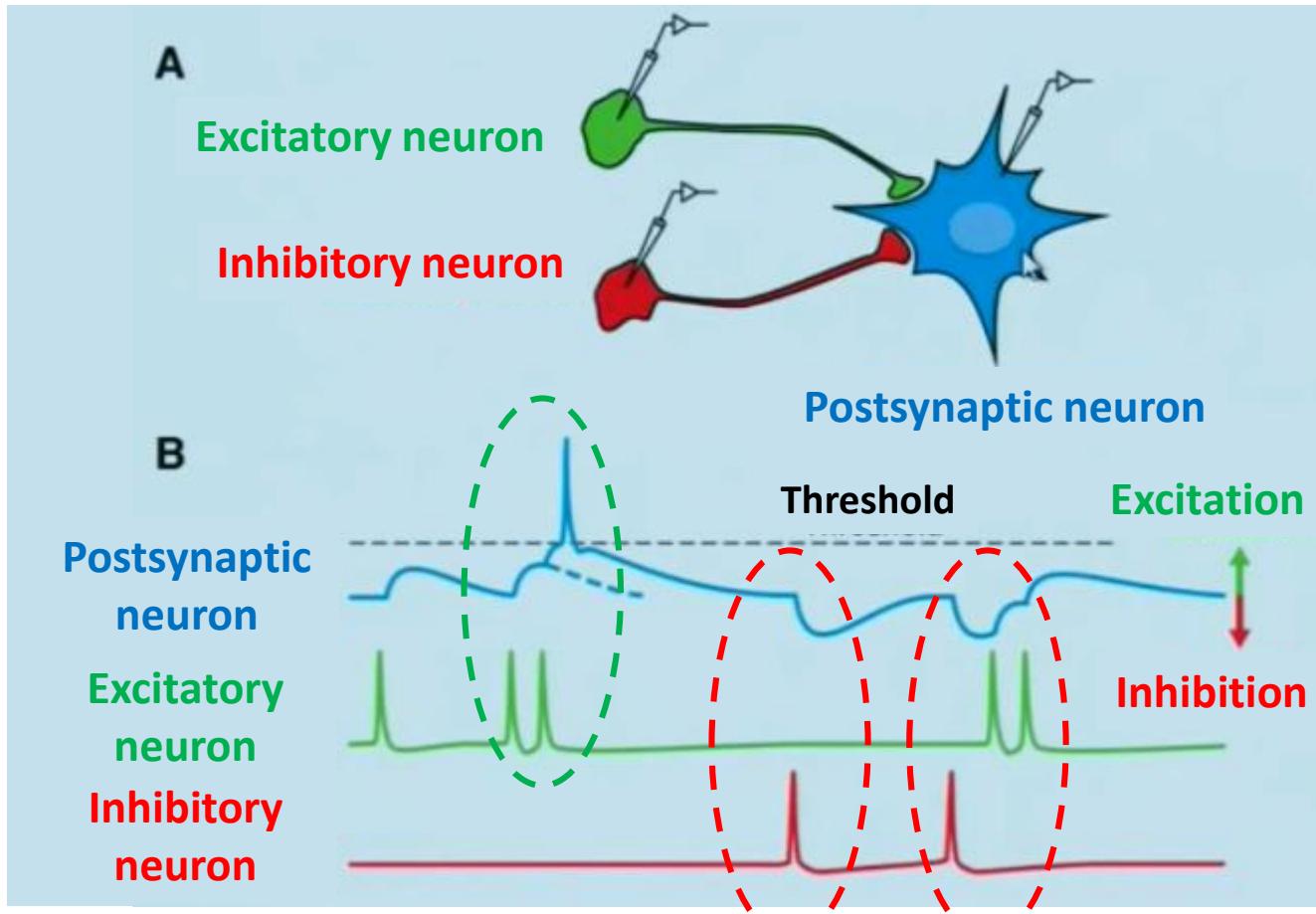


# Modeling A Neuron

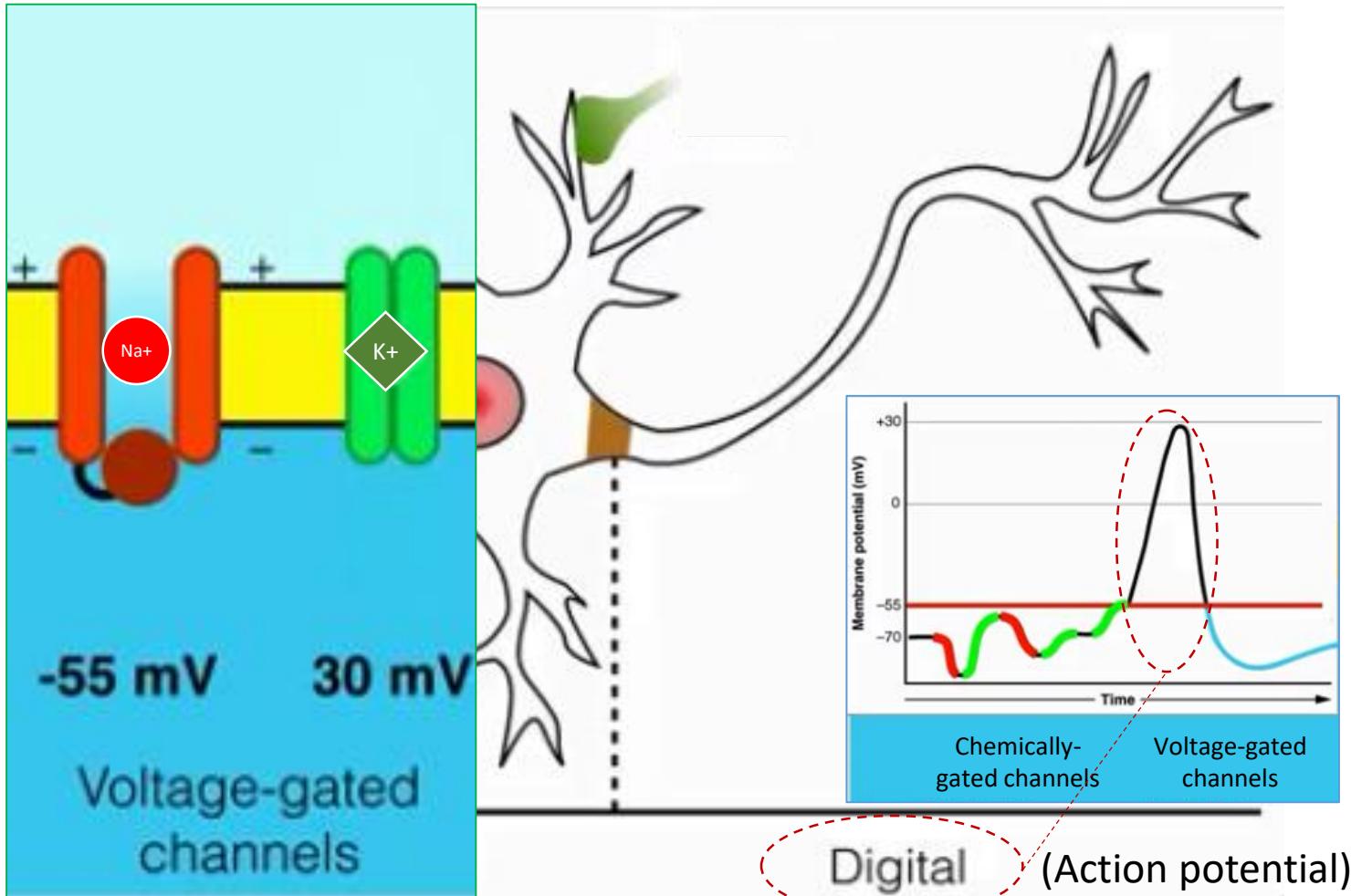
- **Integrate and fire model:** A neuron takes a weighted sum of its inputs and fires a spike if the sum exceeds a threshold



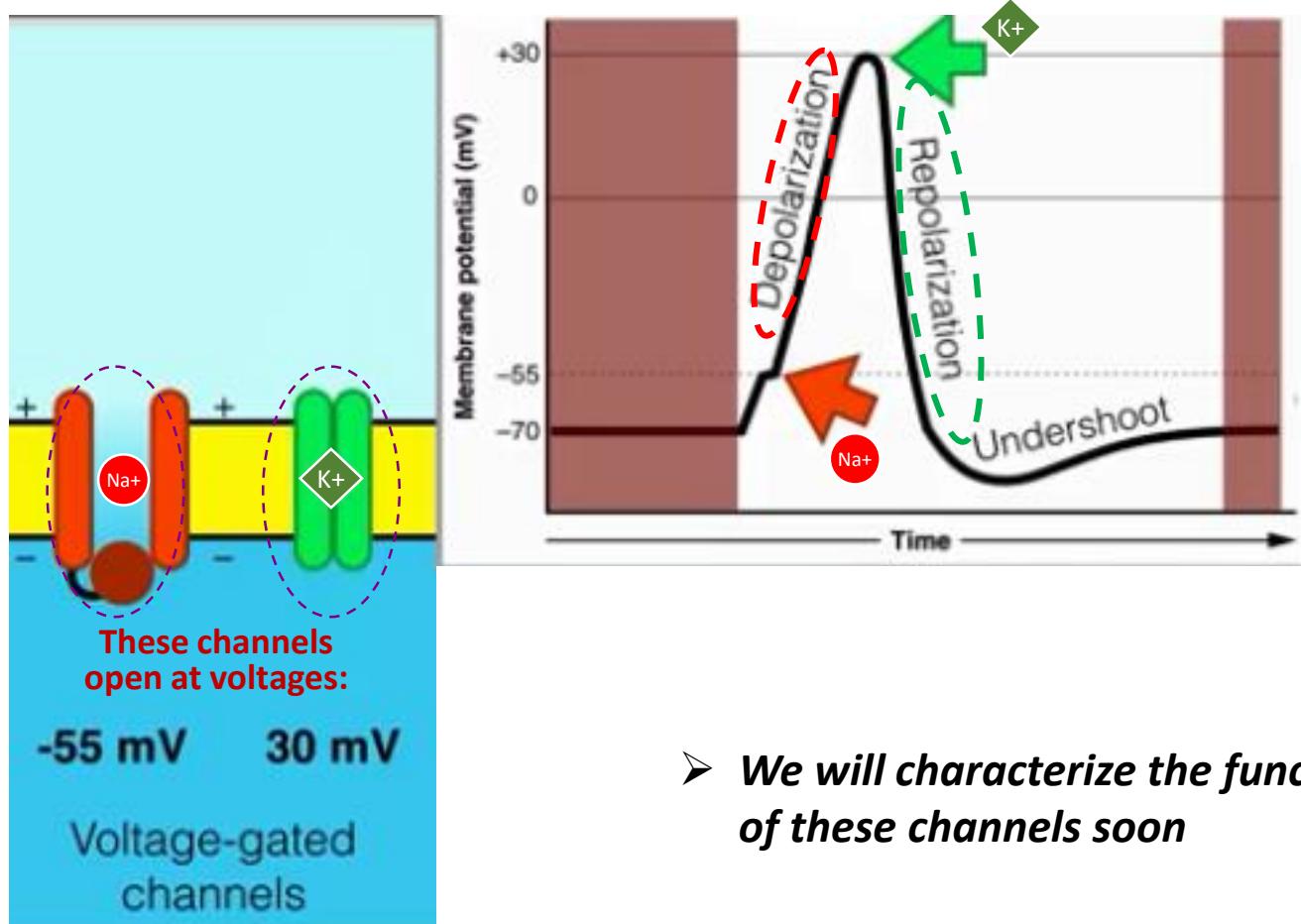
# Ionic Channels – Chemically-Gated Channels (Synapses)



# Ionic Channels – Voltage-Gated Channels (Action Potential)



# Ionic Channels – Voltage-Gated Channels (Action Potential)

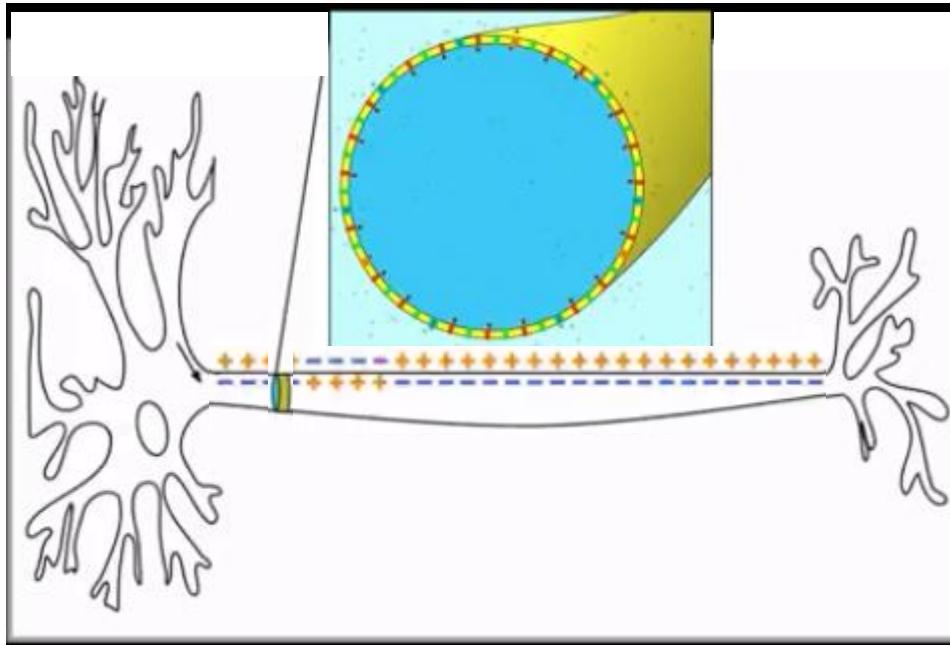


- We will characterize the function of these channels soon

<https://www.youtube.com/watch?v=HYLyhXRp298>  
*(Video to watch later)*

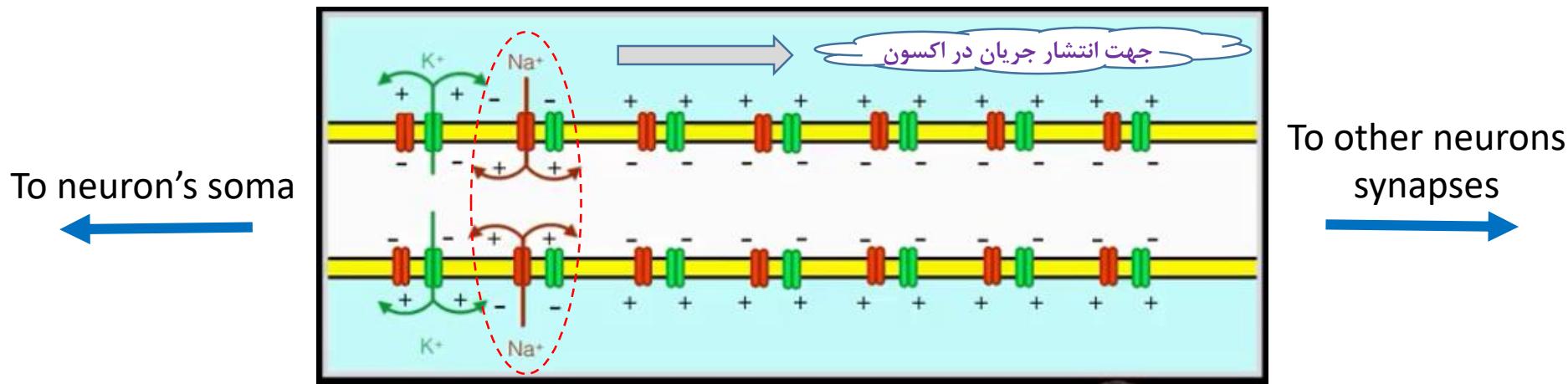
# Axon – Transmission of Action Potential

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- The action potential moves across the axon
- This is performed by:
  - Voltage-gated  $Na^+$  and  $K^+$  channels
  - The role of myelin cover

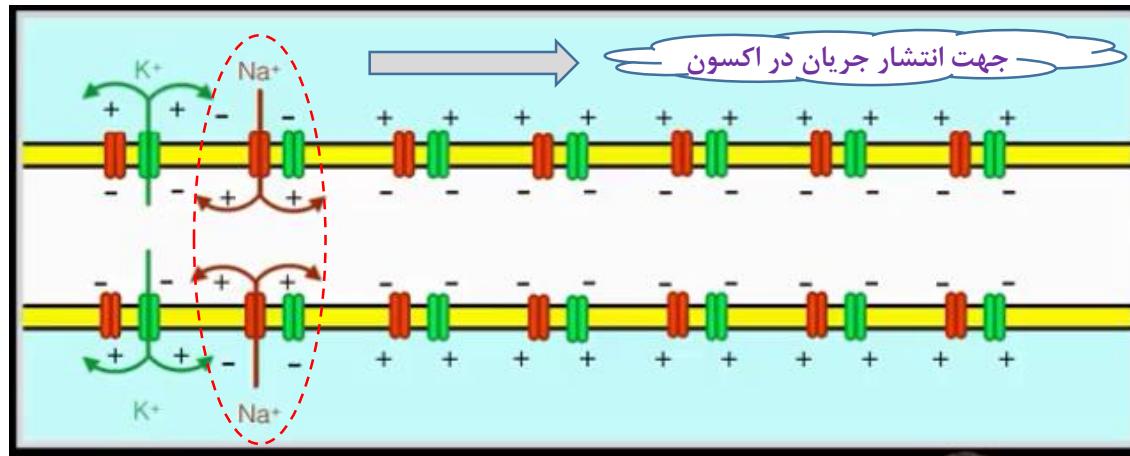
# Axon – Transmission of Action Potential



- As the activation threshold is reached, sodium channels open
- The  $\text{Na}^+$  ions move away from each other due to their charges
  - The charges moving down the axon cause voltage increase  
→ The subsequent sodium channels open
  - Charges moving the other way do not cause any effect (since potassium channels have opened there causing voltage drop)

# Axon – Transmission of Action Potential

To neuron's soma

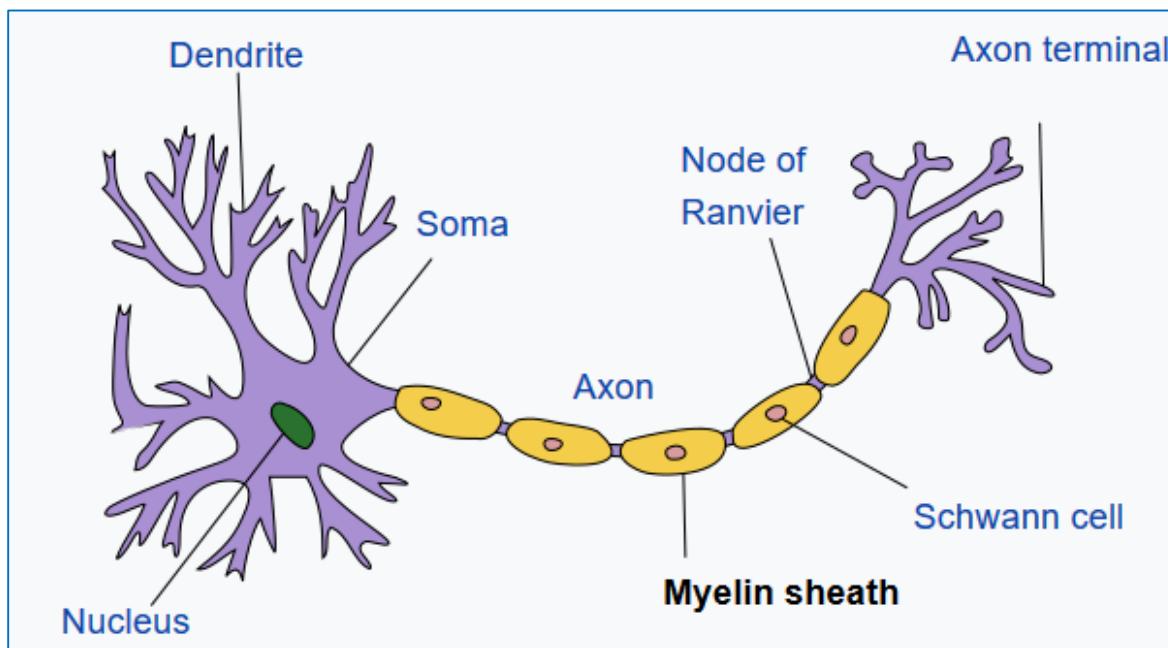


To other neurons  
synapses

- Given the length of a typical axon, and the large number of channels:
  - The transmission of action potential along the axon will be slow (causing long delays in transmission of data or commands across neuronal networks)

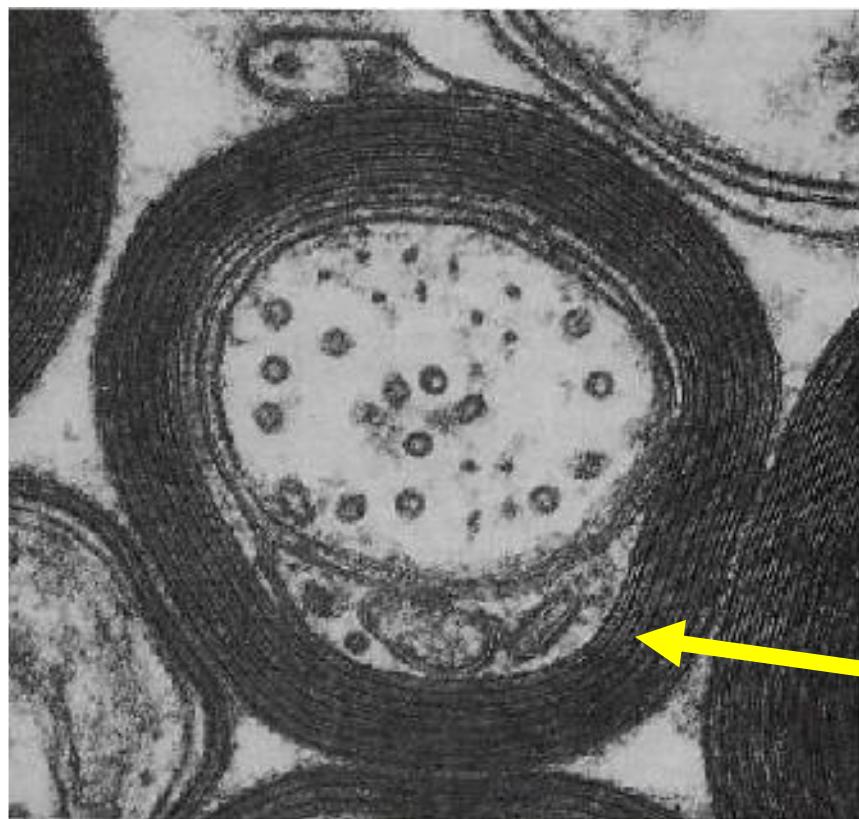
# Active Wiring: Myelination of Axon

- Many axons in vertebrates are covered with an insulating sheath of *myelin*



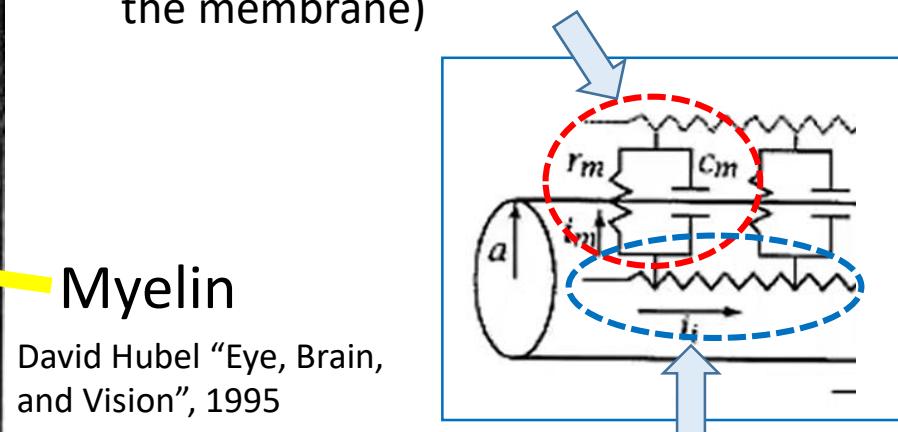
# Active Wiring: Myelination of Axon

The myelin sheath consists of many layers of glial cell membrane wrapped around the axon:



This results in:

- A very high membrane resistance (to prevent passage of charges through the membrane)
- A small membrane capacitance (to prevent accumulation of charges on the membrane)

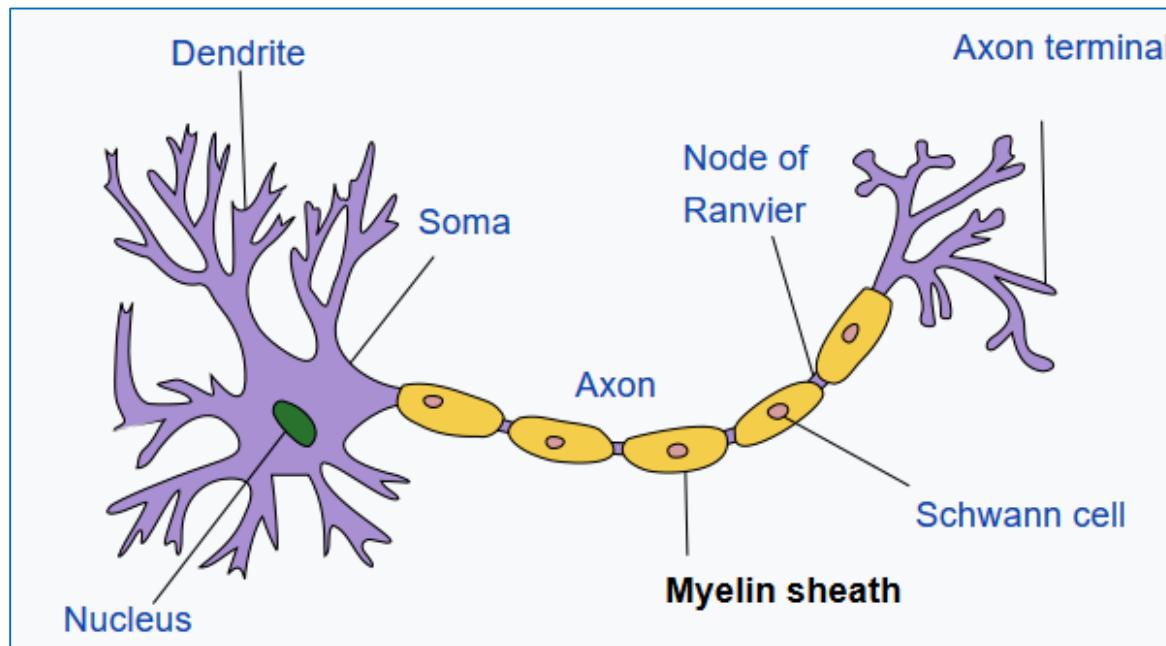


Myelin speeds nerve impulses by promoting charges to travel along the axon

But the voltage drops along the axon <sup>31</sup>

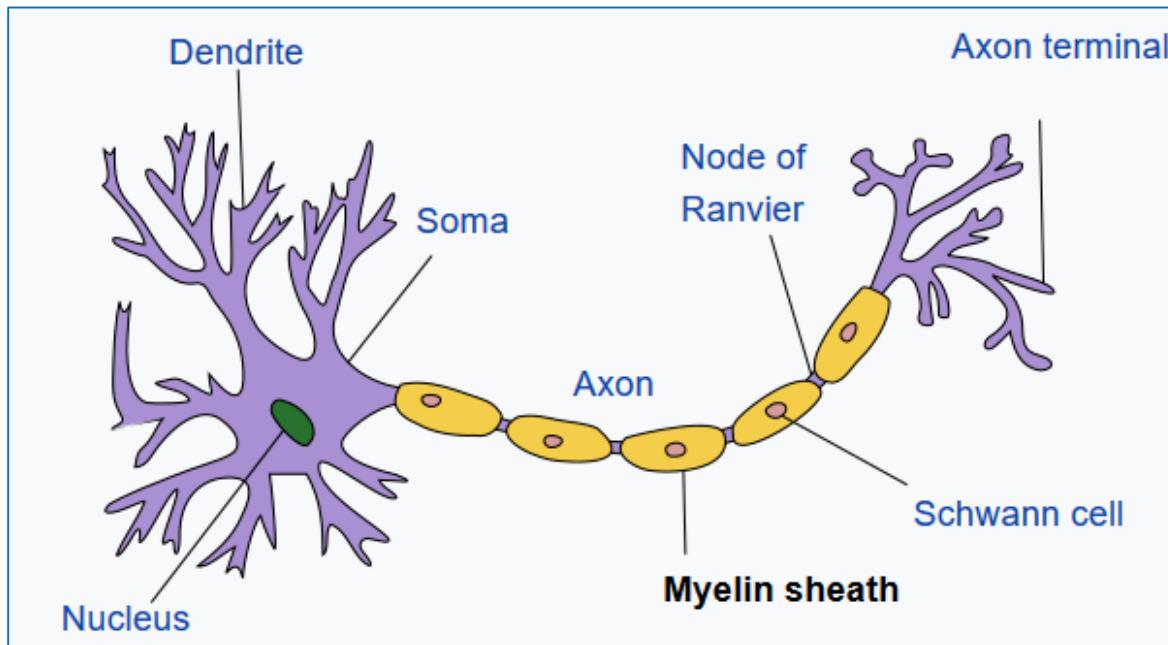
# Active Wiring: Myelination of Axon

- Many axons in vertebrates are covered with an insulating sheath of *myelin*
  - Myelin covers the axon except at gaps (called the *nodes of Ranvier*)
  - There is a high density of fast voltage-dependent Na<sup>+</sup> channels at these nodes



# Active Wiring: Myelination of Axon

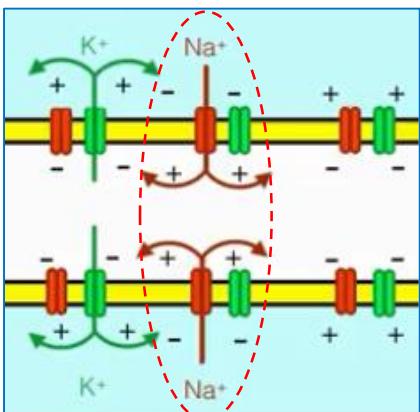
- ***Propagation of action potential:***
  1. Membrane's potential depolarization is transferred **passively** down the myelin-covered sections of the axon  
**(This is fast transmission since it does not involve chemical channels)**



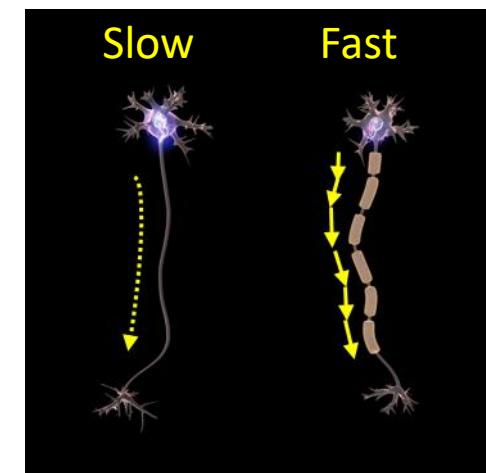
# Active Wiring: Myelination of Axon

- ***Propagation of action potential:***

1. Membrane's potential depolarization is transferred **passively** down the myelin-covered sections of the axon  
**(This is fast transmission since it does not involve chemical channels, but the voltage drops due to resistance to moving charges along the axon)**
2. Action potentials are **actively** regenerated at the nodes of Ranvier  
**(This compensates for the voltage drop caused by passive transmission in myelinated axon regions)**



- This type of transfer is slow
- It only occurs at the nodes of Ranvier

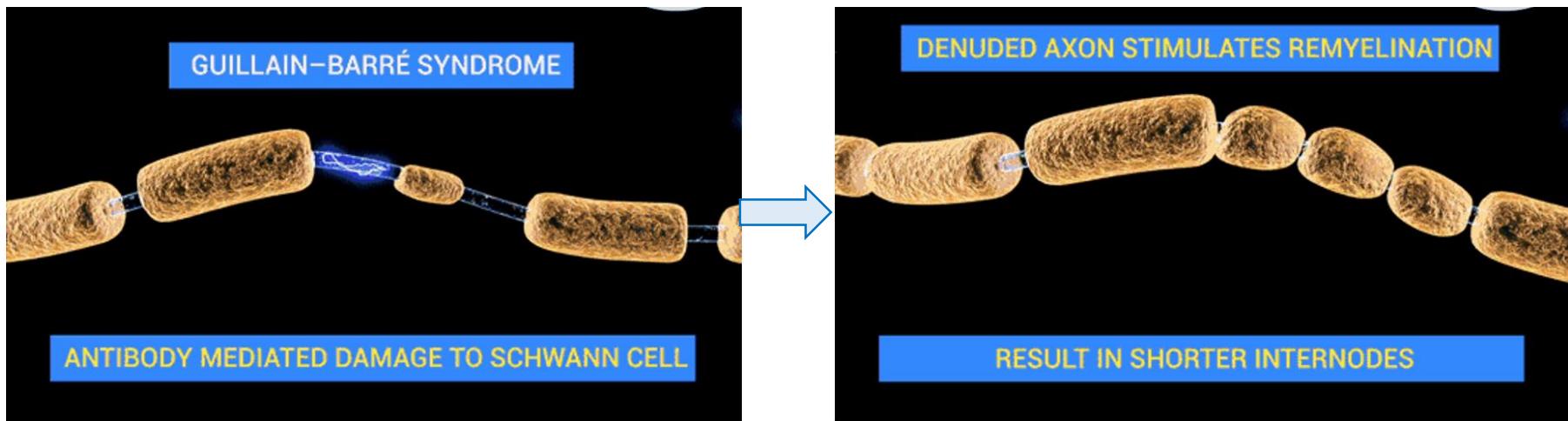


Wikipedia Dr. Jana

# Active Wiring: Myelination of Axon

*Extra Info*

- In **MS (multiple sclerosis)**, the body's auto-immune response damages the myelin, causing the neurons to lose efficient communication



- **Guillain–Barré syndrome (GBS)** is a rapid-onset muscle weakness as a result of damage to the peripheral nervous system

# Outline

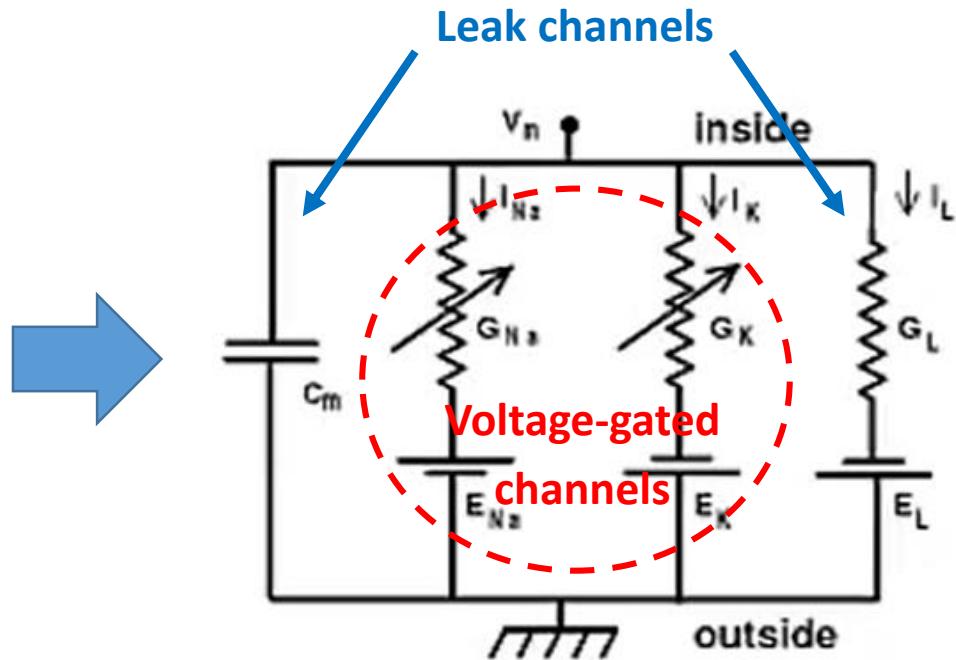
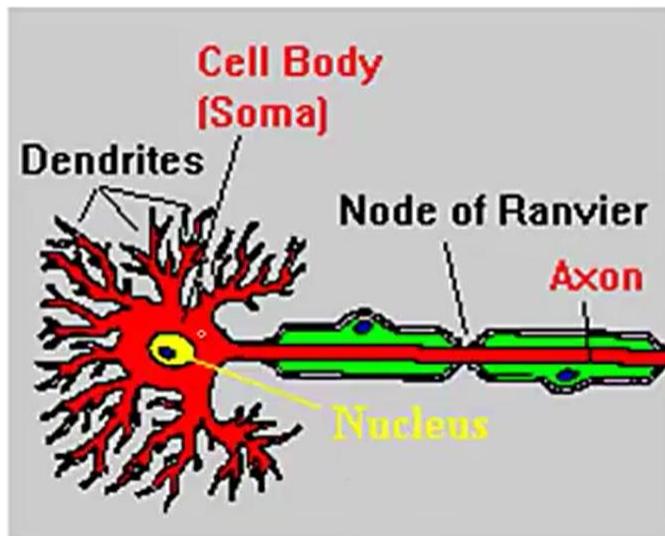
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- Sensing & perception
  - Neurons in the brain
  - Visual cortex & receptive fields
  - Vision & perception
- Neurons & spikes
  - Electrical personality of a neuron
  - Ionic channels
  - Action potential
- The Hodgkin-Huxley equation
  - The passive membrane
  - Voltage-gated channels
  - Anatomy of a spike
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  - Phase portrait models
  - Fixed points and their stability
  - Bifurcation (saddle-node / Hopf)
  - Simplified 2D models

# The Passive Membrane

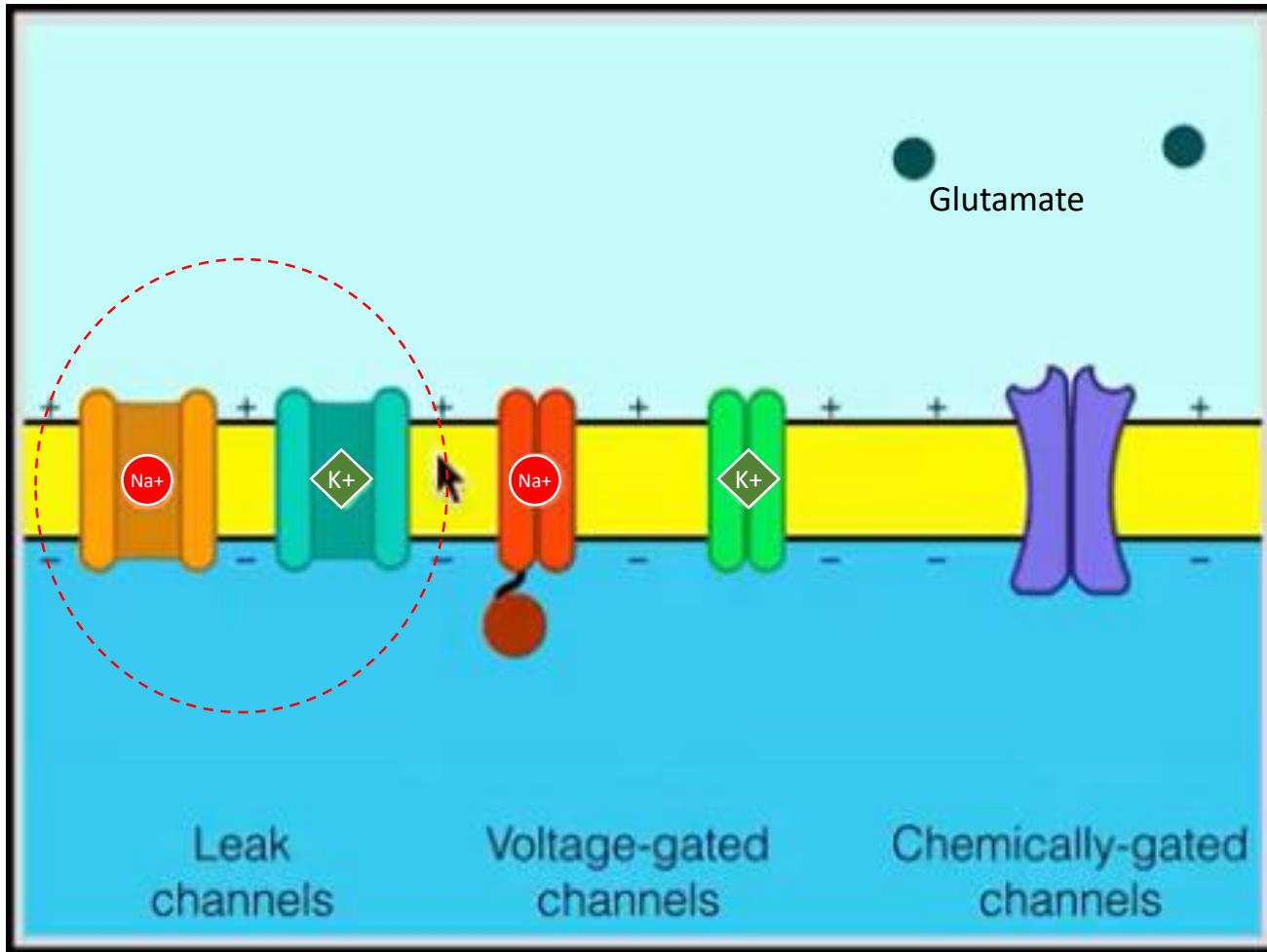
Passive  
Membrane

# Equivalent Circuit Model



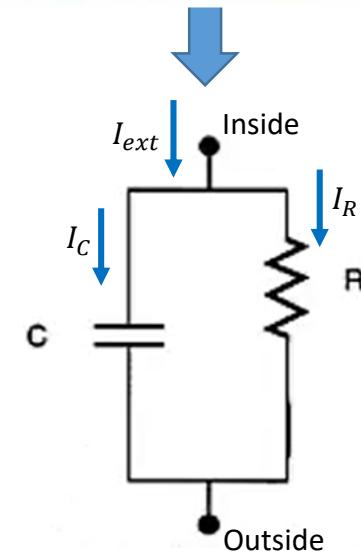
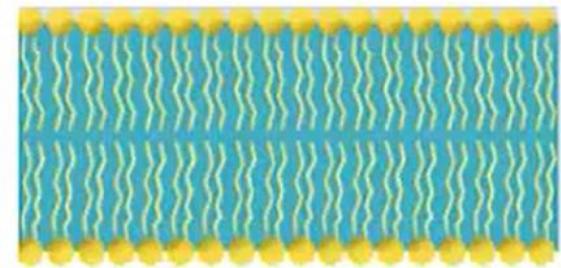
- We will derive a model for the function of a neuron
- The mathematical tool will be differential equations
- Hodgkin and Huxley won nobel prize for deriving such a model

# Ionic Channels – Passive Membrane and Leak Channels



# The Passive Membrane

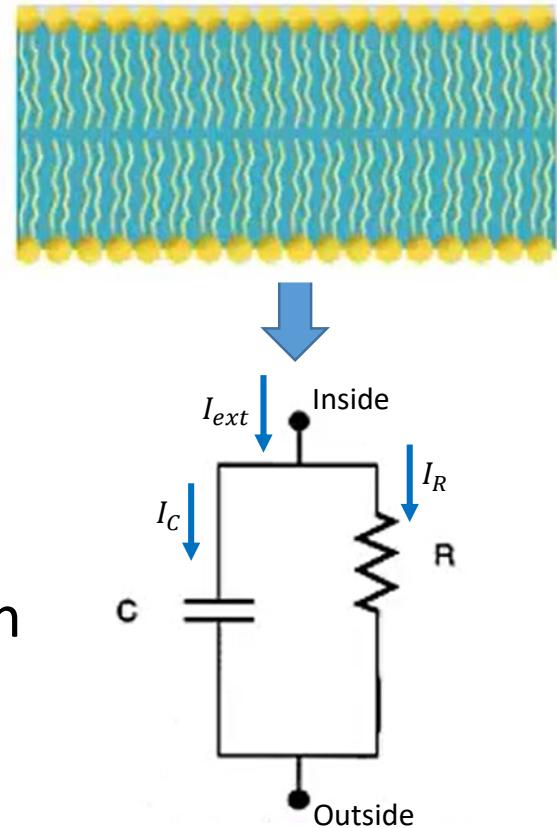
- We will first derive a model for the current that leaks through the membrane itself:
  - The lipid bilayer acts like a **capacitor**
  - Some charge pass through, which can be modeled as a conductance by a **resistor**



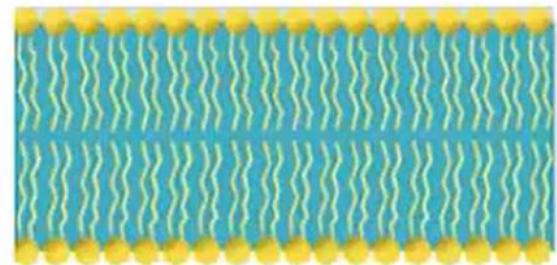
# RC Circuits

- At a junction of wires, the total (input/output) current is zero
- The potential changes by a fixed amount across a battery symbol
- The potential across a resistor is proportional to the current going through it (Ohm's law:  $V = IR$  or  $I = Vg$ )
- The current through a capacitor is proportional to the derivative of the potential across it:

$$I_C = \frac{dQ}{dt} = C \frac{dV}{dt}$$



# The Passive Membrane

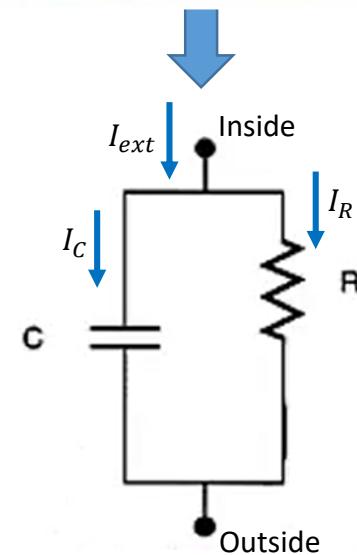


At the node:  $I_{ext} = I_C + I_R$

Ohm's law:  $V = I_R R$

For capacitor:  $C = Q/V$

$$I_C = \frac{dQ}{dt} = C \frac{dV}{dt}$$

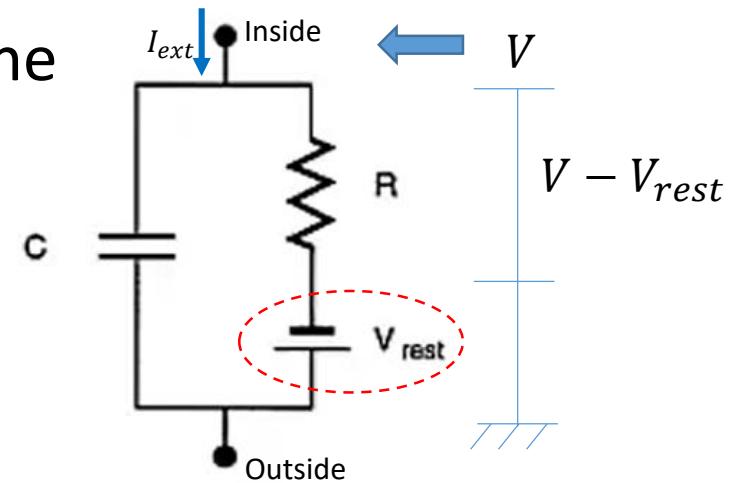
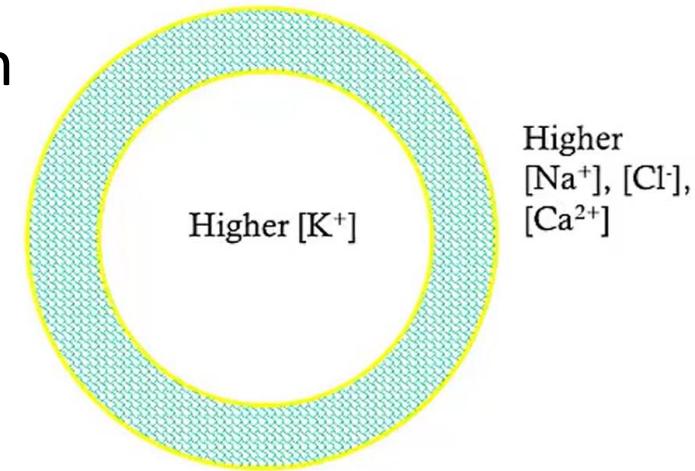


$$C \frac{dV}{dt} = -\frac{V}{R} + I_{ext}$$

# Leak Channels – The Cell Has A Battery

- The membrane encloses a solution in which concentrations of ions are different from outside
- This difference in ion concentrations can be modeled by a **potential difference**  $V_{rest}$  across the membrane

$$C \frac{dV}{dt} = -\frac{(V - V_{rest})}{R} + I_{ext}$$

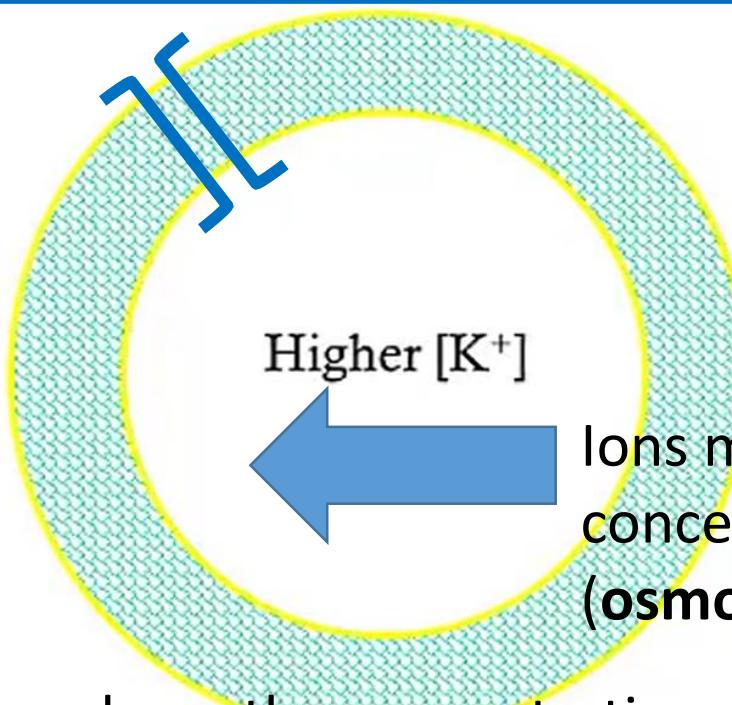


➤ *Let's see how this potential difference is derived*

# Leak Channels – The Cell Has A Battery

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Until opposed by  
**electrostatic forces**

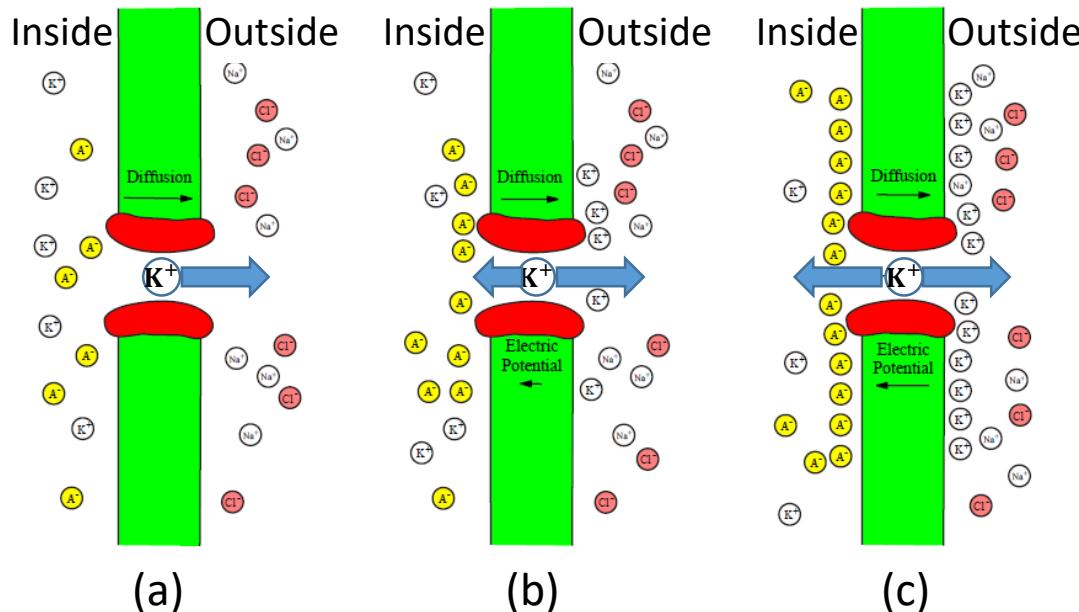


Higher  
 $[Na^+]$ ,  $[Cl^-]$ ,  
 $[Ca^{2+}]$

Ions move down their  
concentration gradient  
(osmosis)

- **Diffusion** of  $K^+$  ions down the concentration gradient through the membrane (due to osmosis)
- This creates an **electric potential** force directed at the opposite direction
- And continues until the diffusion and electrical forces **counter each other**

# Leak Channels – The Cell Has A Battery

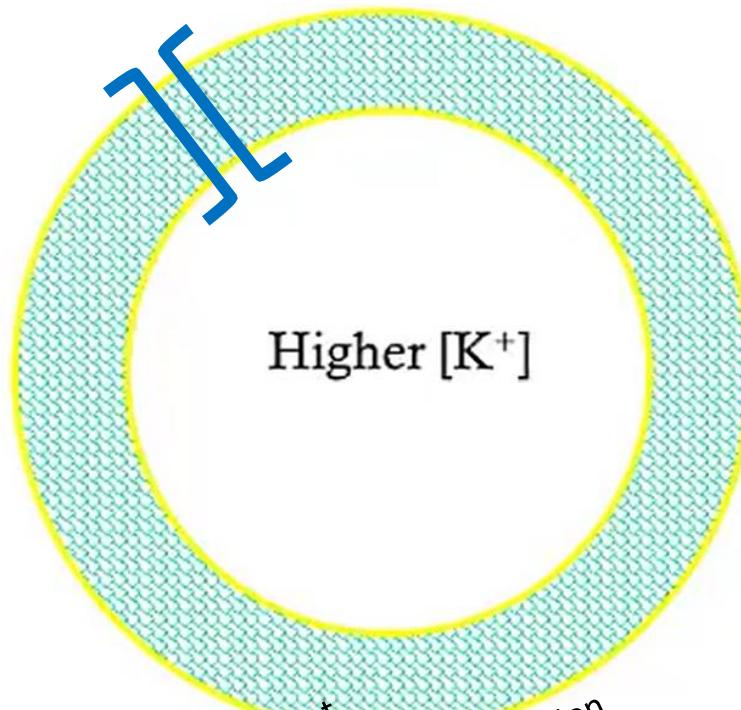


- The resulting transmembrane potential is referred to as **Nernst equilibrium potential** for  $K^+$
- Each ion type has its own equilibrium potential (i.e. if only that ion was allowed to diffuse through the membrane)
  - Resulting in an equivalent potential (the neuron's resting potential) about **-70 mV**

$$\begin{aligned}E_{Na} &\sim 50 \text{ mV} \\E_{Ca} &\sim 150 \text{ mV} \\E_K &\sim -80 \text{ mV} \\E_{Cl} &\sim -60 \text{ mV}\end{aligned}$$

# Leak Channels – The Cell Has A Battery

*Extra Info*



At equilibrium:

$$\text{Nernst potential: } E = \frac{K_B T}{z q} \ln \frac{[\text{inside}]}{[\text{outside}]} = \frac{V_T}{z} \ln \frac{[\text{inside}]}{[\text{outside}]}$$

Boltzman's constant  
Temperature  
Ion concentration  
inside  
No. of protons  
Charge of proton  
Ion concentration  
outside

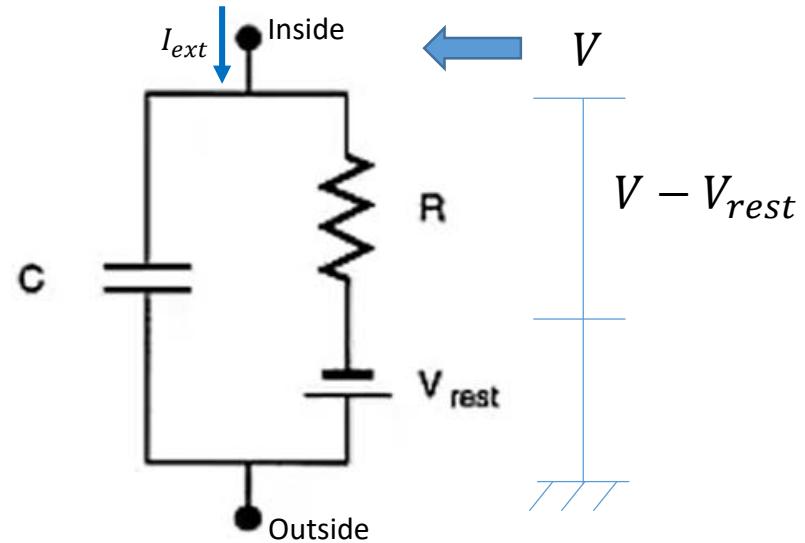
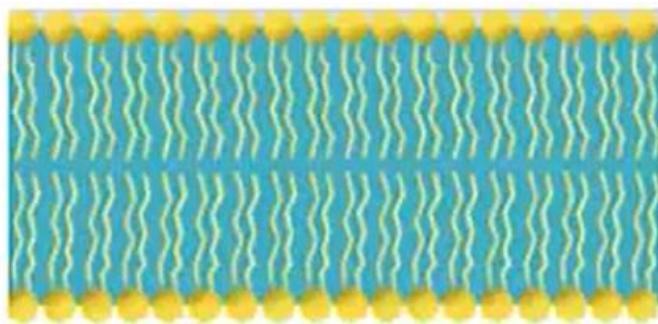
(This equilibrium potential is calculated for each ion type)

$V_T$  is around 24-27 mV

$E_{Na} \sim 50 \text{ mV}$   
 $E_{Ca} \sim 150 \text{ mV}$   
 $E_K \sim -80 \text{ mV}$   
 $E_{Cl} \sim -60 \text{ mV}$

# Leak Channels – The Cell Has A Battery

- The voltage drop across the resistor is decreased by the amount  $V_{rest}$  (i.e. it will be  $V - V_{rest}$ )



$$C \frac{dV}{dt} = -\frac{(V - V_{rest})}{R} + I_{ext}$$

# Leak Channels – The Cell Has A Battery

- Let's compare the form of the differential equation with a familiar form:

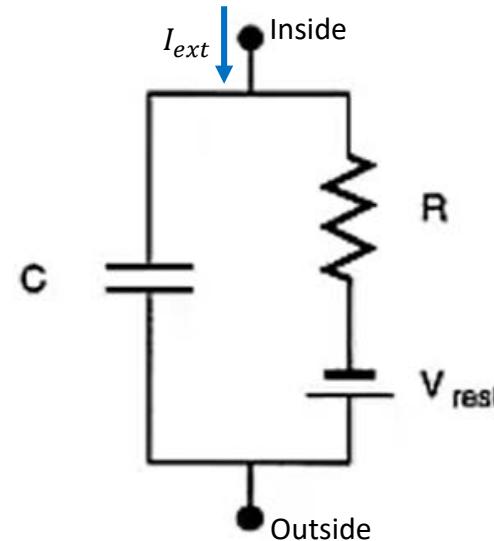
$$C \frac{dV}{dt} = -\frac{(V - V_{rest})}{R} + I_{ext}$$

Define:

$$\tau = RC$$

$V_\infty$ : steady state solution

$$\left( \frac{dV}{dt} = 0 \right) \rightarrow V_\infty = V_{rest} + RI_{ext}$$



$$\tau \frac{dV}{dt} = -V + V_\infty , \quad V_\infty = V_{rest} + RI_{ext}$$

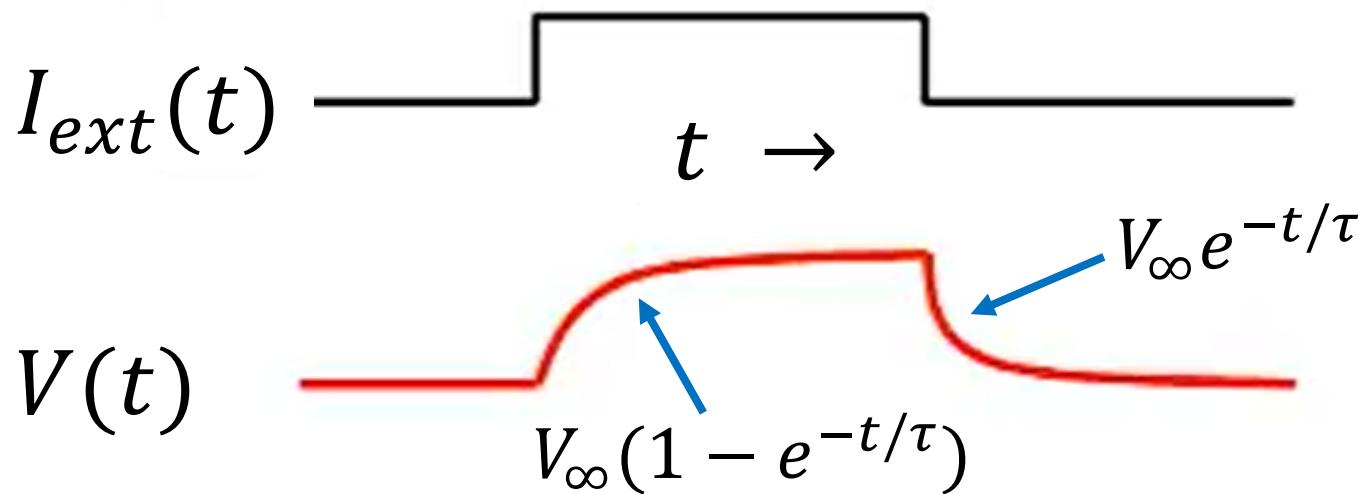
# Leak Channels – The Cell Has A Battery

---

$$\tau \frac{dV}{dt} = -V + V_\infty$$

$$V_\infty = V_{rest} + RI_{ext}$$

- For an input current in the form of a pulse:

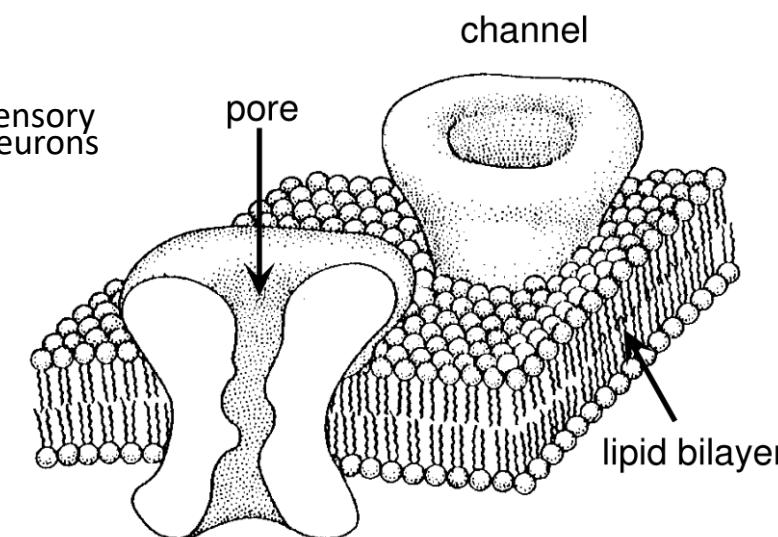


# Voltage-gated Channels

Channels  
Voltage-gated

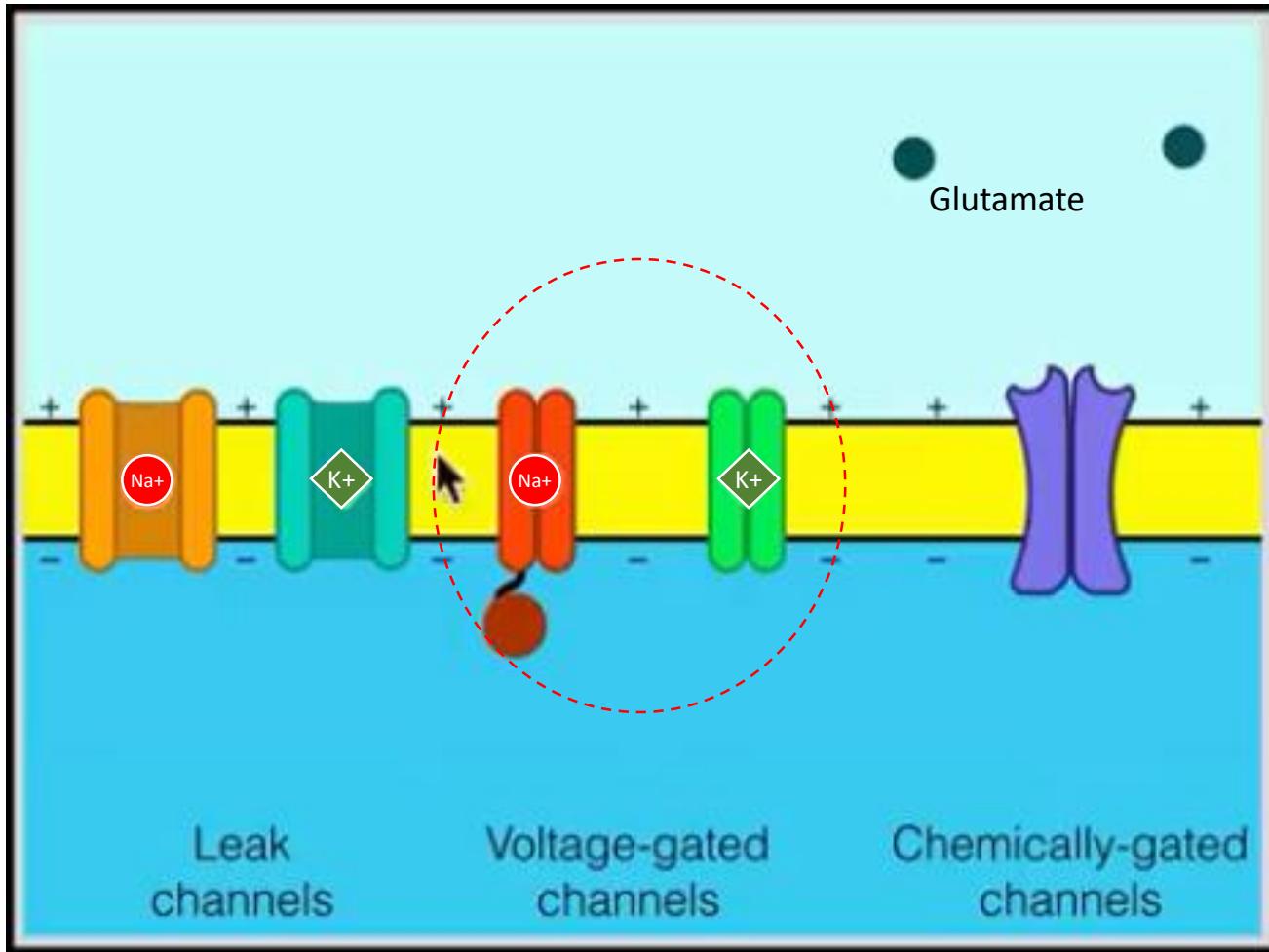
# Currents Flow through Ion Channels

- Ion channels distinguish between different ions  
→ Different ions have different rates of transport between inside and outside the neuron
- Ion channels are of many types:
  - Neurotransmitter-dependent (synaptic) ←(we'll model these later)
  - Voltage-dependent ←(we'll first learn about these)
  - Ca-dependent
  - Mechanosensitive
  - Heat sensitive



# Ionic Channels – Voltage-Gated Channels

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# Voltage-Gates Channels – A Battery for Each Ion Type

- Different ion channels have associated **conductances**
- A given conductance tends to move the membrane potential toward the equilibrium potential for that ion

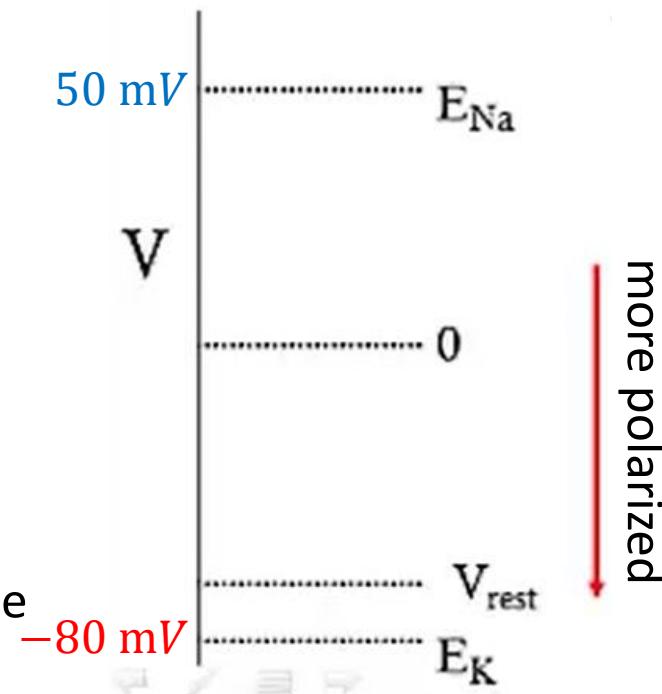
$$E_{Na} \sim 50 \text{ mV}$$

$$E_{Ca} \sim 150 \text{ mV}$$

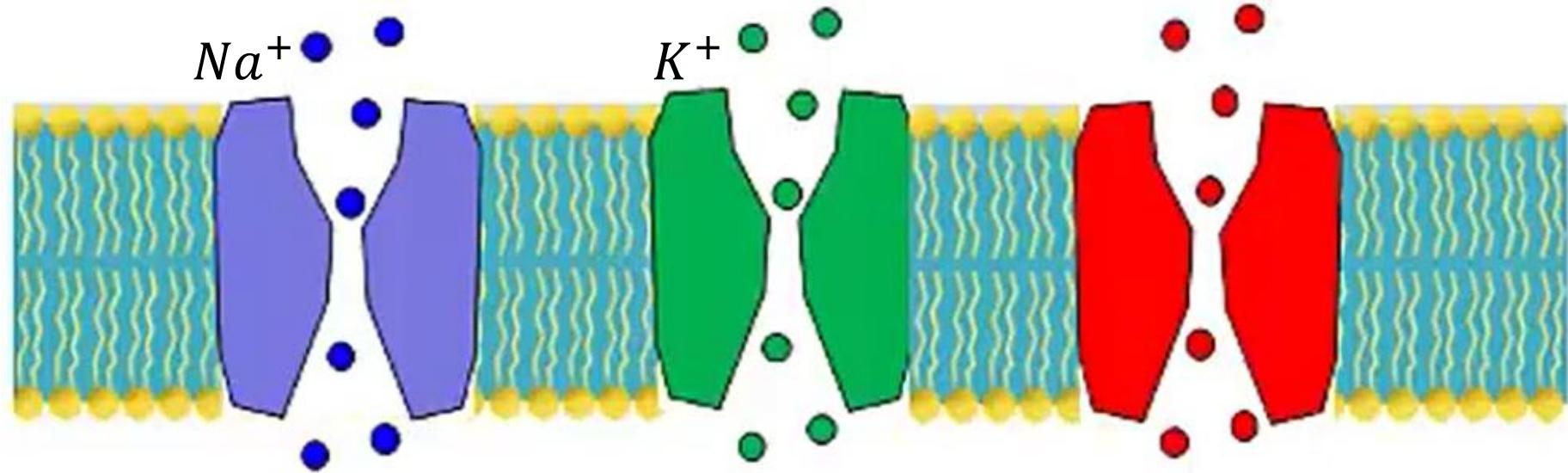
$$E_K \sim -80 \text{ mV}$$

$$E_{Cl} \sim -60 \text{ mV}$$

- We will focus on *Na* and *K* currents:
  - *Na* current tends to **depolarize** the membrane  
(i.e. move it towards more positive potentials)
  - *K* current tends to **hyperpolarize** the membrane  
(i.e. move it towards more negative potentials)

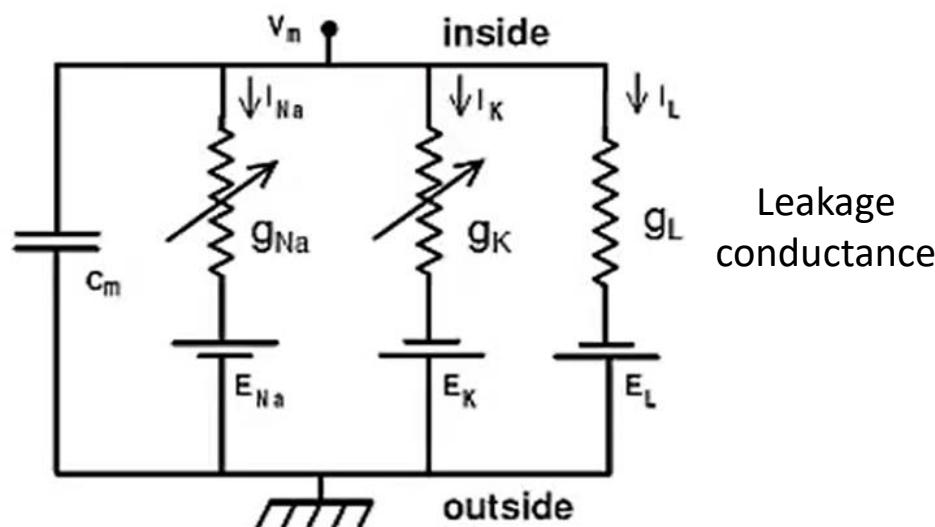


# Equivalent Circuit Model



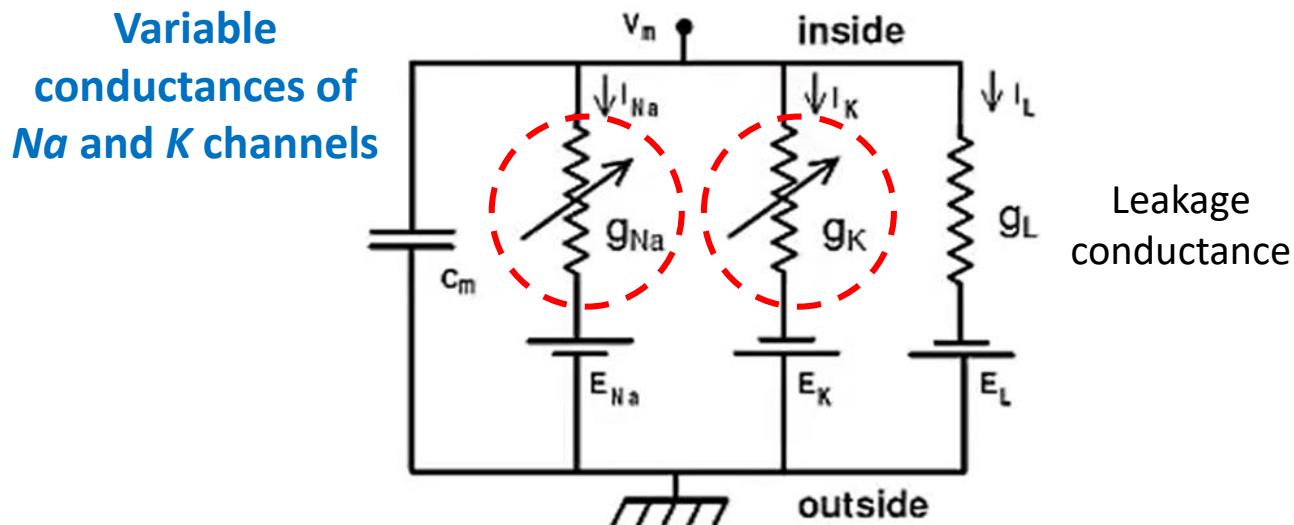
Parallel paths for different ions:

$$I_i = g_i(V - E_i)$$



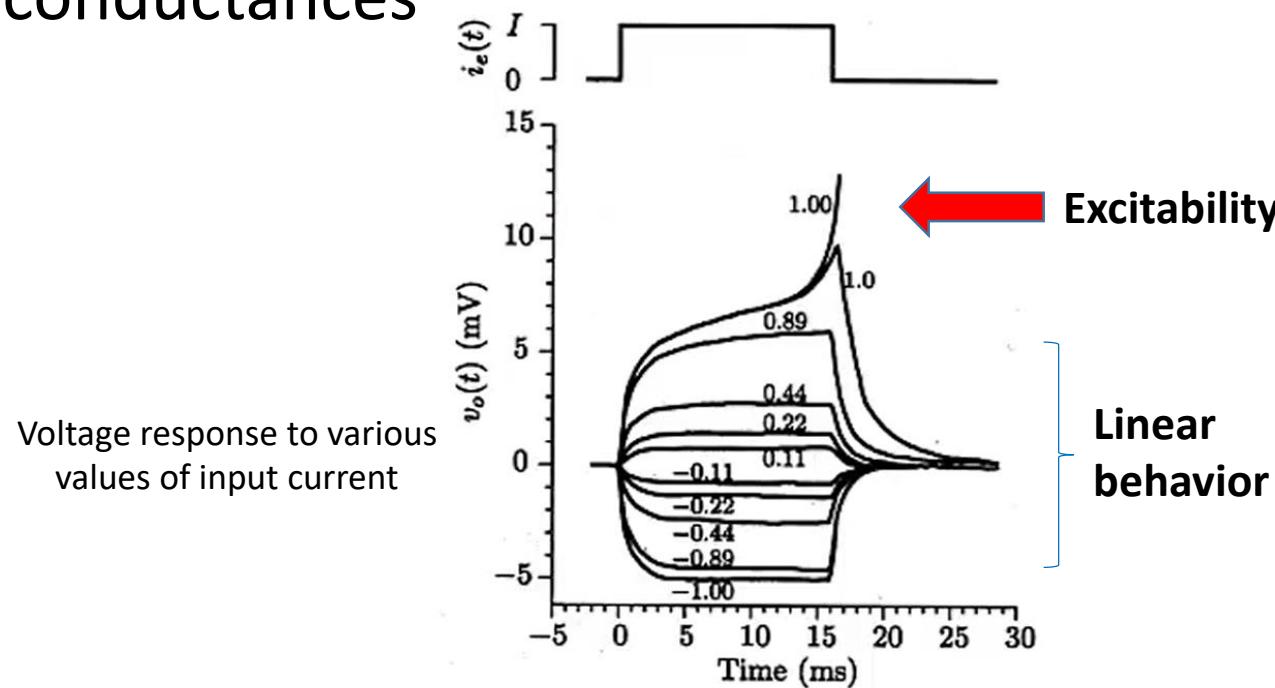
# Equivalent Circuit Model

- The variable conductances associated with the ion channels make the model much more interesting



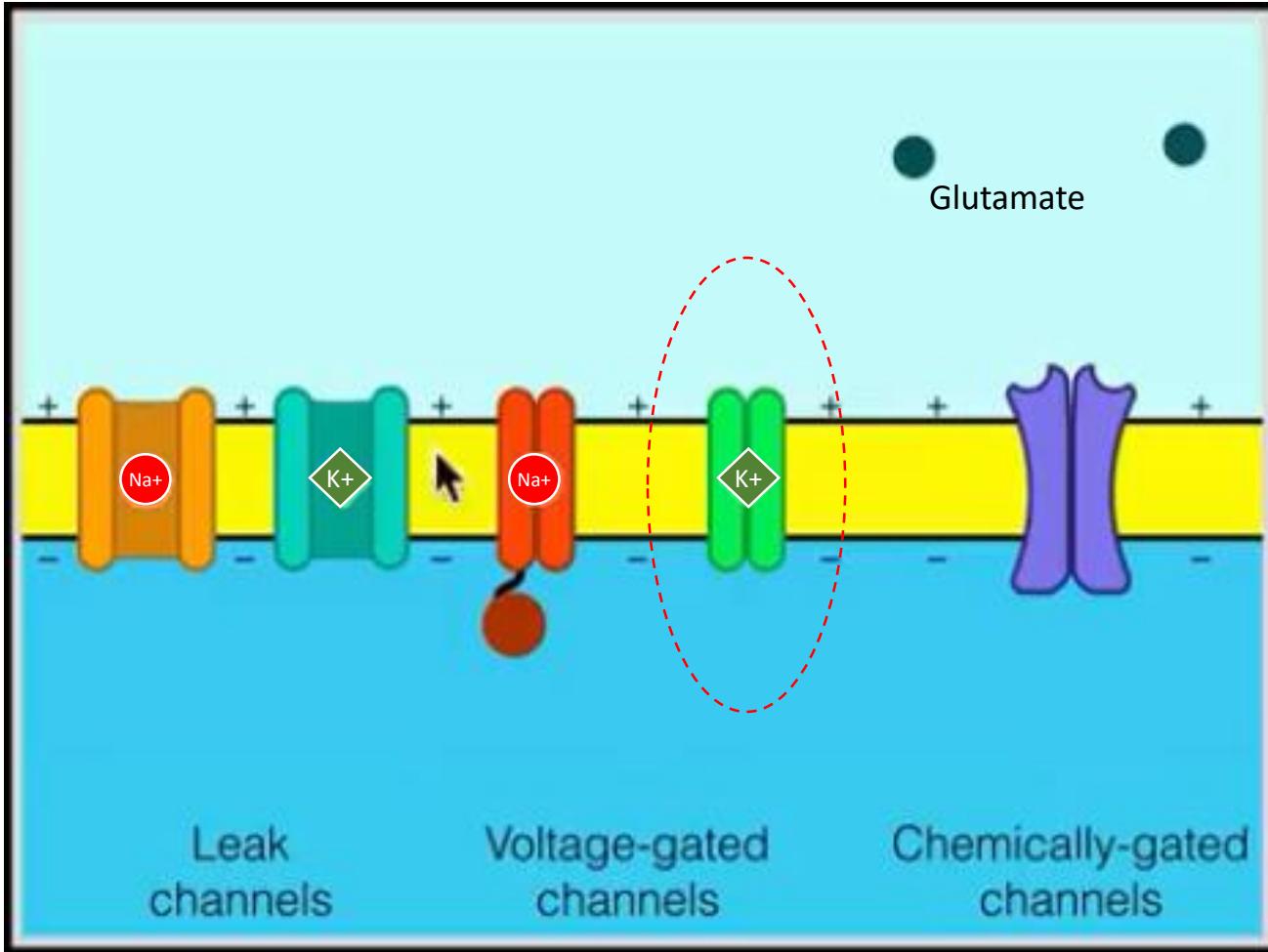
# What Makes a Neuron To Compute?

- Instead of producing a linear response to the input, the neuron responds in an interesting fashion
- This is due to the *nonlinearities* of the ion channel conductances

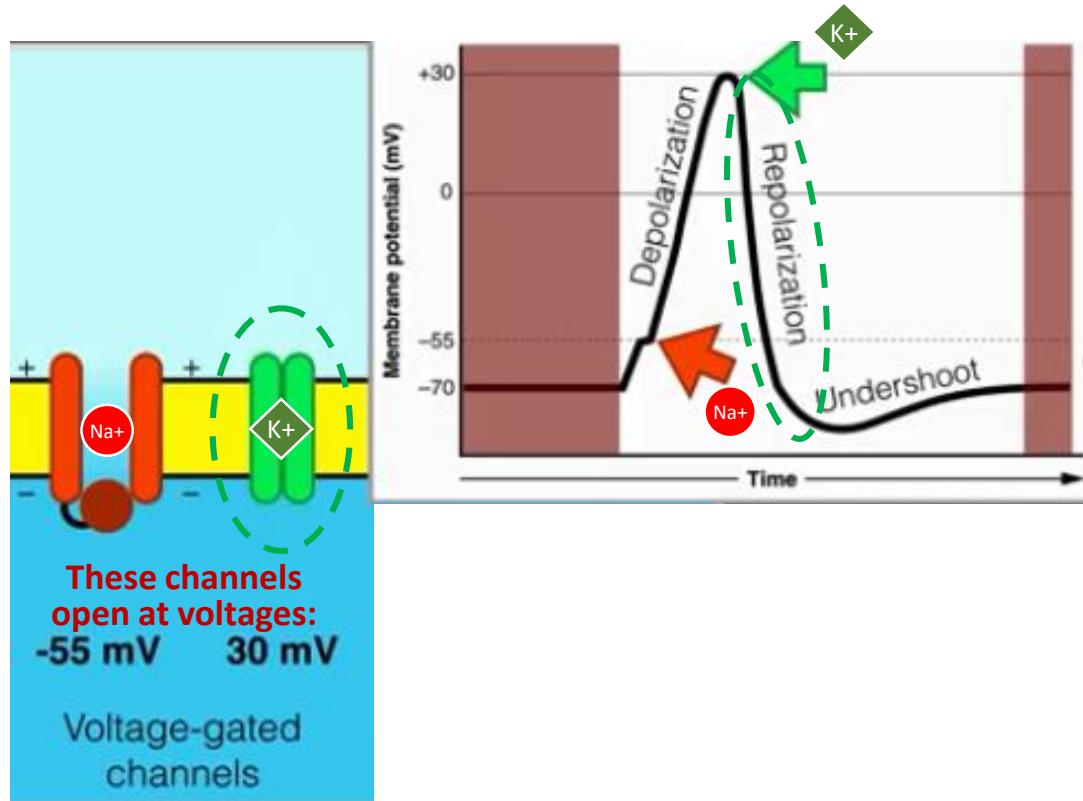


➤ We will see how the nonlinear behavior leads to spiking

# Voltage-Gated Channels – The Potassium Channel

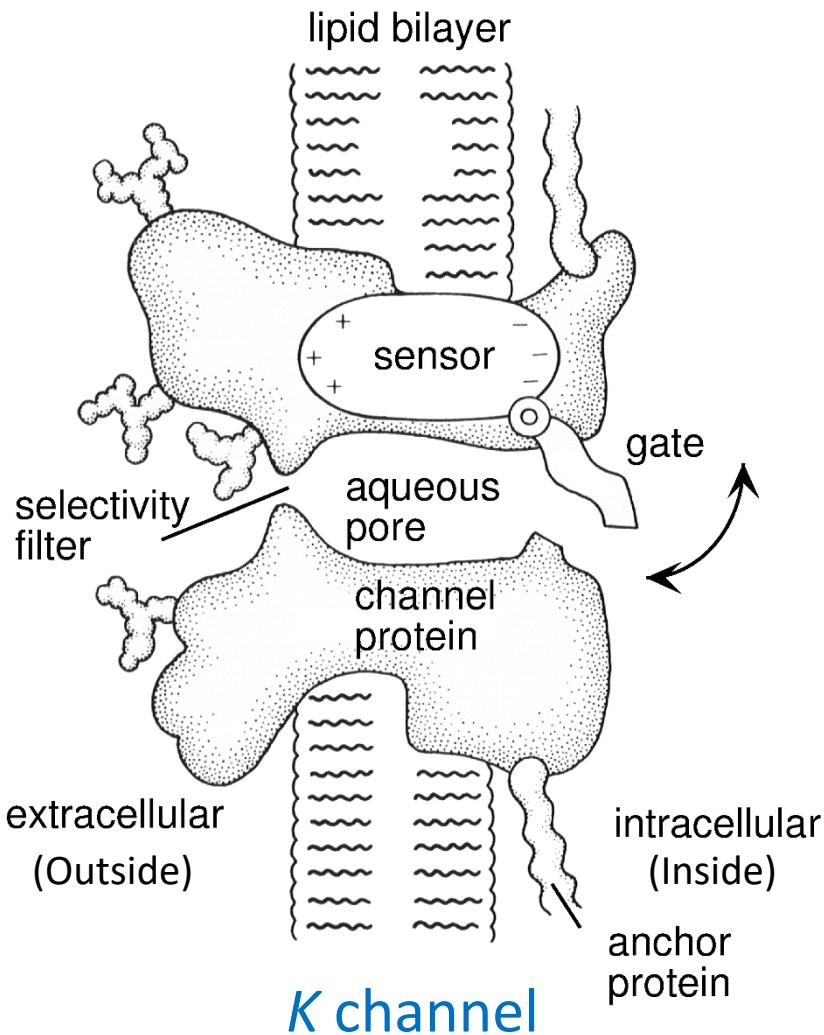


# Voltage-Gated Channels – The Potassium Channel



# The Potassium Channel – A Cool Molecular Machine

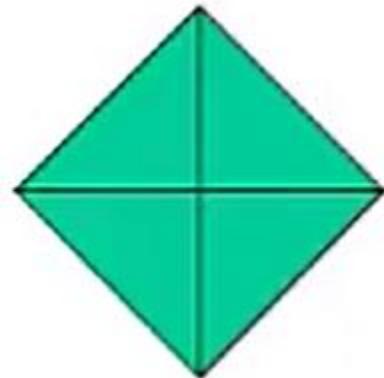
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- The potassium channel contains:
  - **A gate:** Controls the entrance of ions
  - **A voltage sensor:** Controls the configuration of the gate
- The probability of **gate open** increases when the neuron is **depolarized** (i.e. with increasing voltage)

# The Potassium Channel – A Cool Molecular Machine

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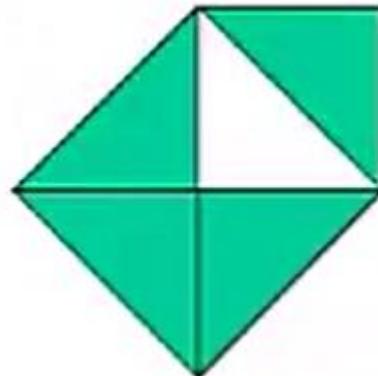
A simplified model  
for the gate

- The gate has 4 sub-units
  - All 4 need to be in the correct configuration for the ions to go through
- Let  $n$  describe the status of a sub-unit:
  - $n$ : open probability
  - $1 - n$ : closed probability
- For the channel to be open (assume independent sub-units):

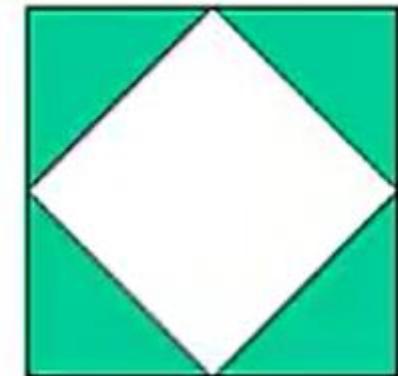
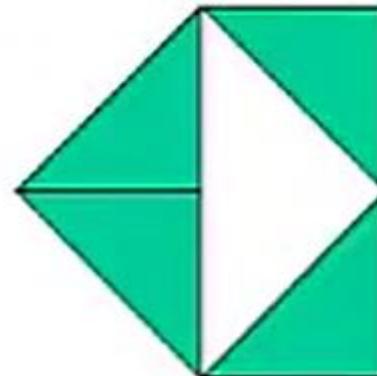
$$P_K \sim n^4$$



One sub-unit open



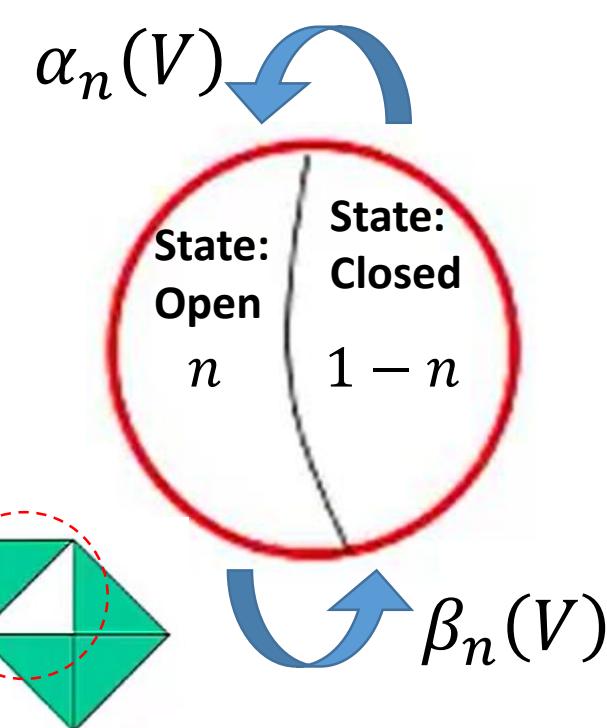
Two sub-units open



All sub-units open

# The Potassium Channel – A Cool Molecular Machine

- To calculate the dynamics of the probability of having a sub-unit open:
  - We need to consider transitions between the states of the sub-unit



- Transitions between states occur at ***voltage-dependent*** rates:

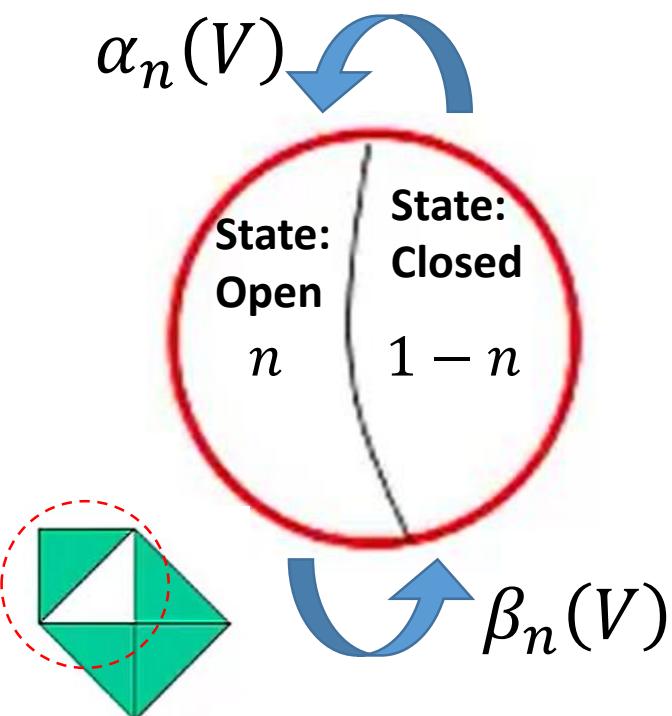
$\alpha_n(V)$ : Rate of transition from **Closed to Open**

$\beta_n(V)$ : Rate of transition from **Open to Closed**

# The Potassium Channel – A Cool Molecular Machine

- Probability that a sub-unit **opens** over a short interval  $\Delta t$ :  $(1 - n) \alpha_n(V)\Delta t$   
Probability of being closed  
x Rate of transition from closed to open  
x Time interval
- Probability that a sub-unit **closes** over a short interval  $\Delta t$ :  $n \beta_n(V)\Delta t$   
Probability of being open  
x Rate of transition from open to closed  
x Time interval
- The **open probability** of a sub-unit **changes** over  $\Delta t$  as:  
$$\Delta n = [\alpha_n(V)(1 - n) - \beta_n(V)n]\Delta t$$
- The **rate** at which the open probability of a sub-unit changes over time:

$$\frac{dn}{dt} = \alpha_n(V)(1 - n) - \beta_n(V)n$$



# The Potassium Channel – A Cool Molecular Machine

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$$\frac{dn}{dt} = \alpha_n(V)(1 - n) - \beta_n(V)n$$

- Rewrite the differential equation in the familiar form:

$$\frac{dn}{dt} = -n(\alpha_n(V) + \beta_n(V)) + \alpha_n(V)$$

(Dividing both sides by  $\alpha_n(V) + \beta_n(V)$ ):



$$\frac{1}{\alpha_n(V) + \beta_n(V)} \frac{dn}{dt} = -n + \frac{\alpha_n(V)}{\alpha_n(V) + \beta_n(V)}$$

- In canonical form:

$$\tau_n(V) \frac{dn}{dt} = -n + n_\infty(V)$$

where:

$$\tau_n(V) = \frac{1}{\alpha_n(V) + \beta_n(V)}$$

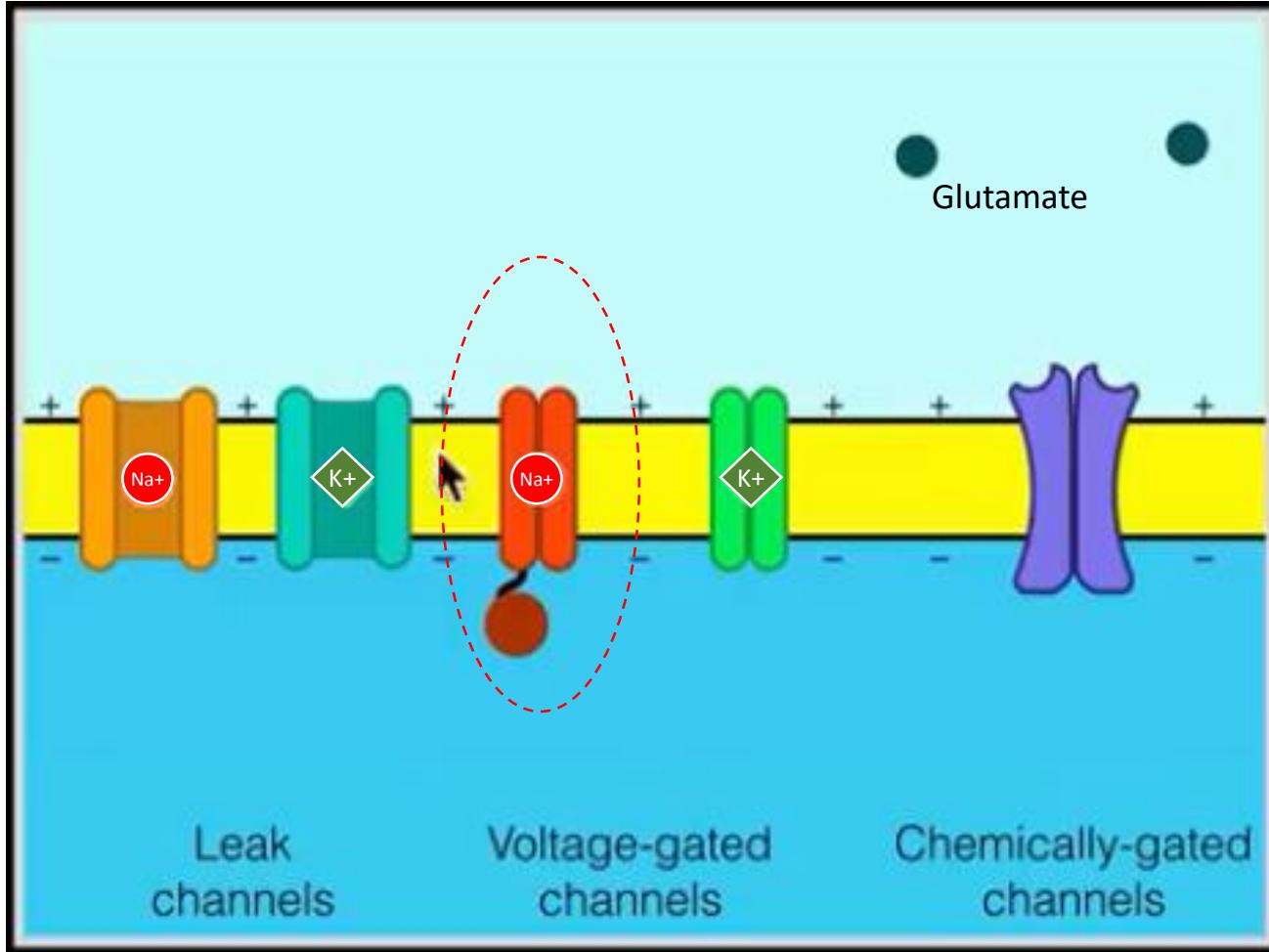
$$n_\infty(V) = \frac{\alpha_n(V)}{\alpha_n(V) + \beta_n(V)}$$

Note:  $n_\infty(V)$  is the steady-state value of  $n$  (when  $\frac{dn}{dt} = 0$ )

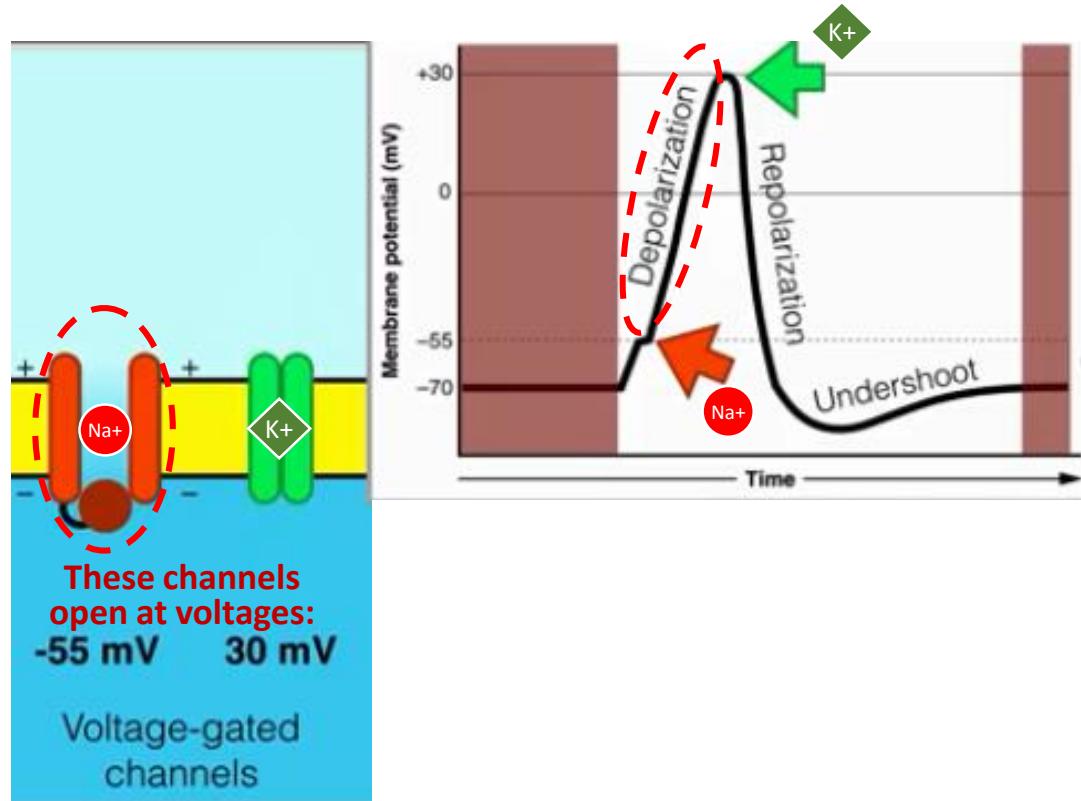
➤ We will next derive a similar model for the sodium channel

# Voltage-Gated Channels – The Sodium Channel

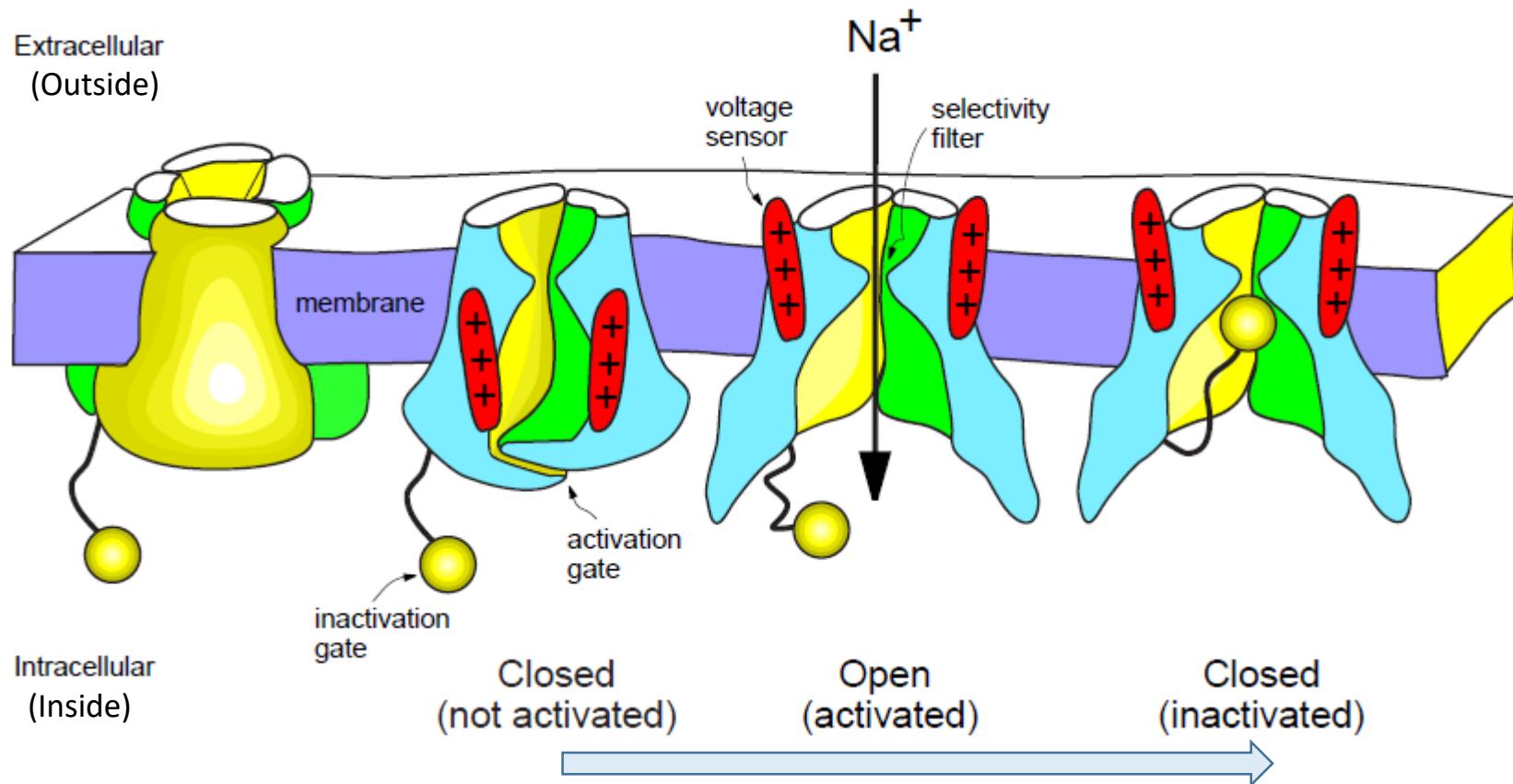
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# Voltage-Gated Channels – The Sodium Channel



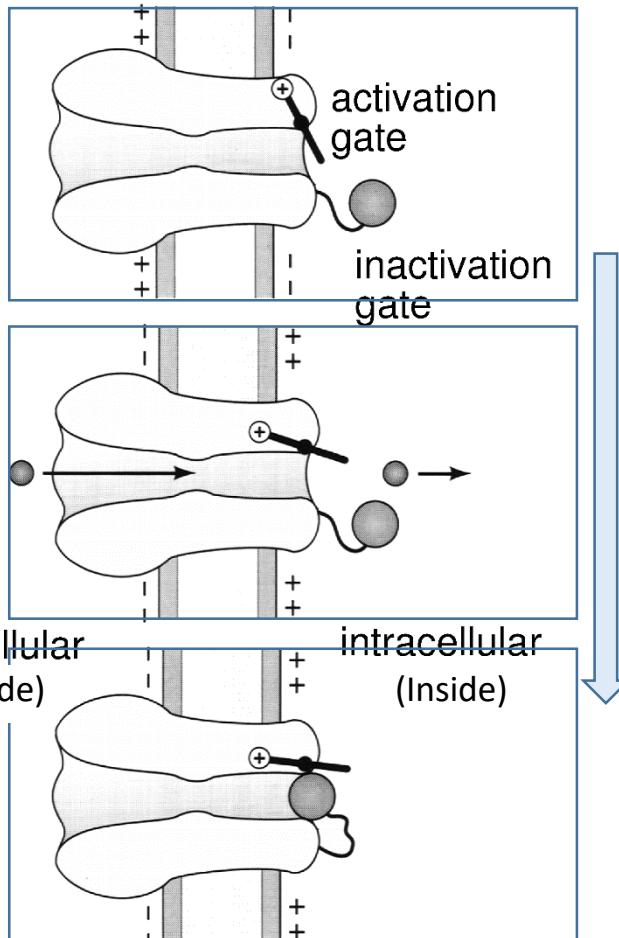
# Voltage-Gated Channels – The Sodium Channel



The sodium channel contains 2 different gates:

- An activation gate
- An inactivation gate

# The Sodium Channel – Transient Conductances



*Na* channel

- The sodium channel contains 2 different gates:
  - **An activation gate:** Controls the entrance of ions (like in the potassium channel) **with 3 sub-units**  
**(Probability of each sub-unit being open:  $m$ )**
  - **An inactivation gate:** An additional gate which can block the channel when closed  
**(Probability of gate being not closed:  $h$ )**
  - For the channel to be open:

$$P_{Na} \sim m^3 h$$

# Dynamics of Activation and Deactivation

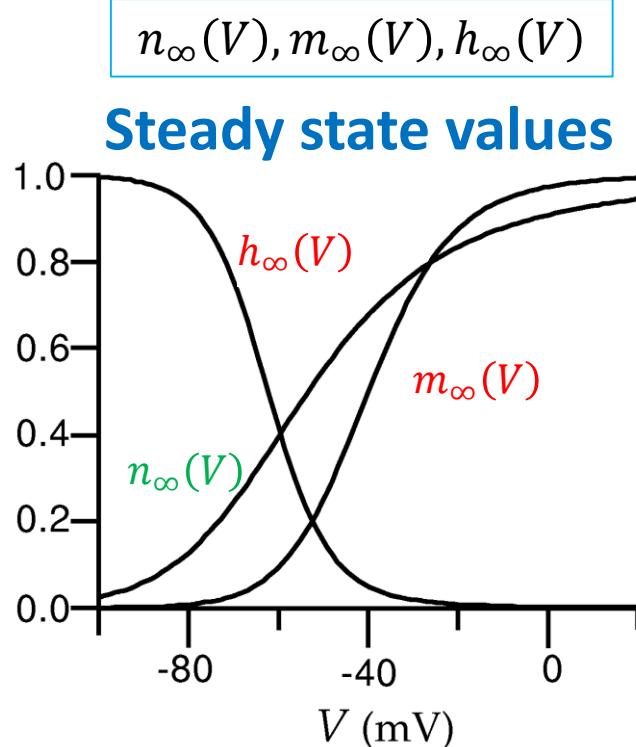
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- we can write canonical forms for the sodium gates  $m$  and  $h$  (in terms of time constants and steady-state values):

$$\tau_m(V) \frac{dm}{dt} = m_\infty(V) - m \quad \tau_m(V) = \frac{1}{\alpha_m(V) + \beta_m(V)}, \quad m_\infty(V) = \frac{\alpha_m(V)}{\alpha_m(V) + \beta_m(V)}$$

$$\tau_h(V) \frac{dh}{dt} = h_\infty(V) - h \quad \tau_h(V) = \frac{1}{\alpha_h(V) + \beta_h(V)}, \quad h_\infty(V) = \frac{\alpha_h(V)}{\alpha_h(V) + \beta_h(V)}$$

# Dynamics of Activation and Inactivation



- $m$  and  $h$  have opposite voltage dependencies:
- Depolarization (voltage increase):
  - Increases  $m$
  - Decreases  $h$

→ There is an activation window for  $Na$  channel

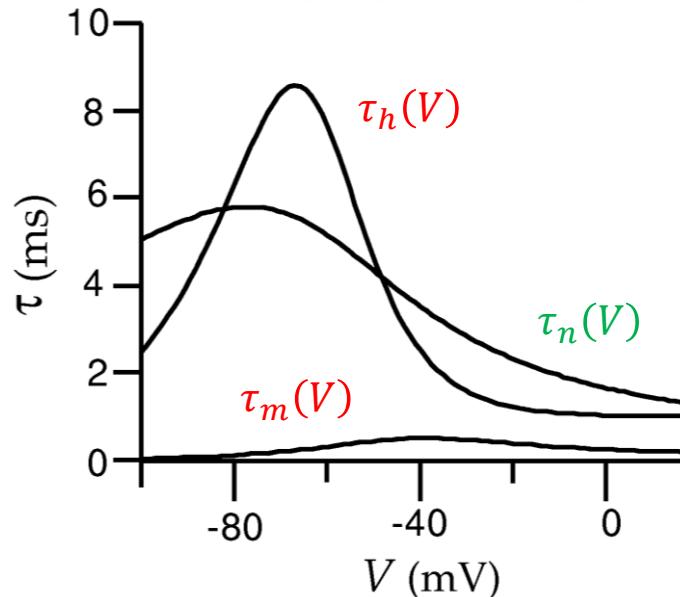
This is where each variable is going with change of voltage

- Activation steady-state values depend on voltage
- They all have sigmoidal forms

# Dynamics of Activation and Inactivation

$$\tau_n(V), \tau_m(V), \tau_h(V)$$

Time constants

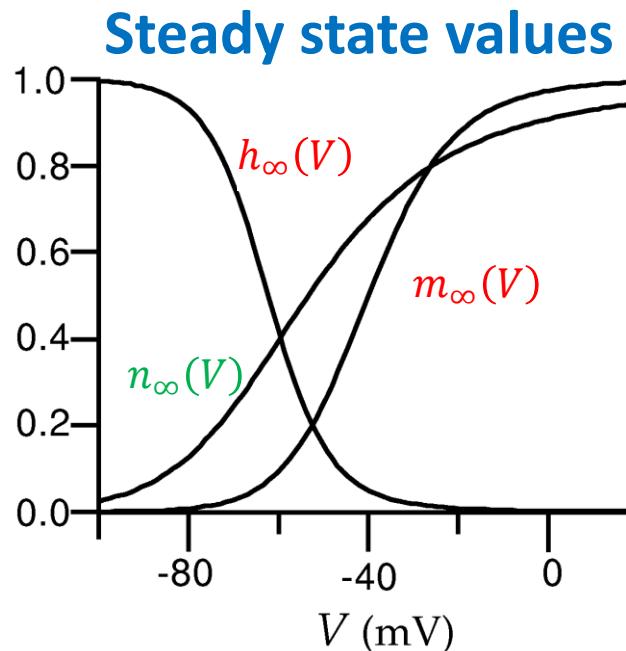


This is how fast it  
gets there

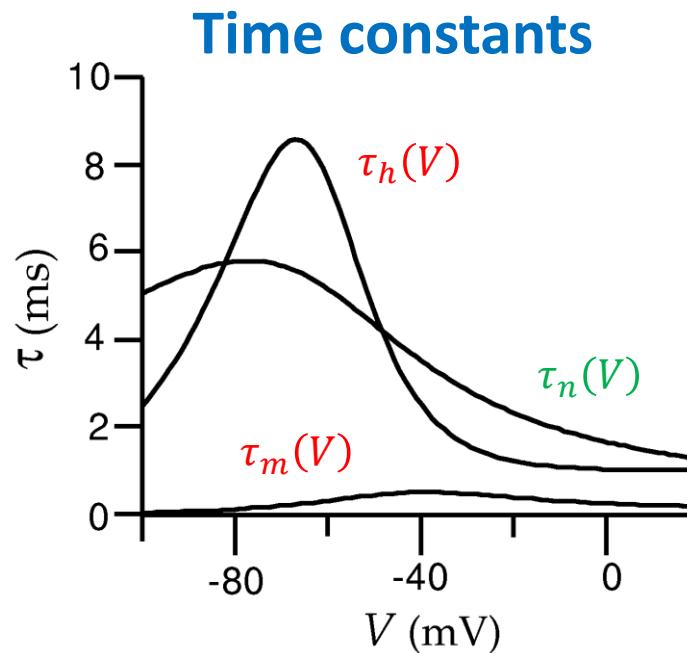
- Time constant values also depend on voltage
- The sodium activation channel  $m$  has the shortest time constant (it rapidly opens with an increase in voltage)

# Dynamics of Activation and Inactivation

$n_\infty(V), m_\infty(V), h_\infty(V)$



$\tau_n(V), \tau_m(V), \tau_h(V)$



This is where each variable is going with change of voltage

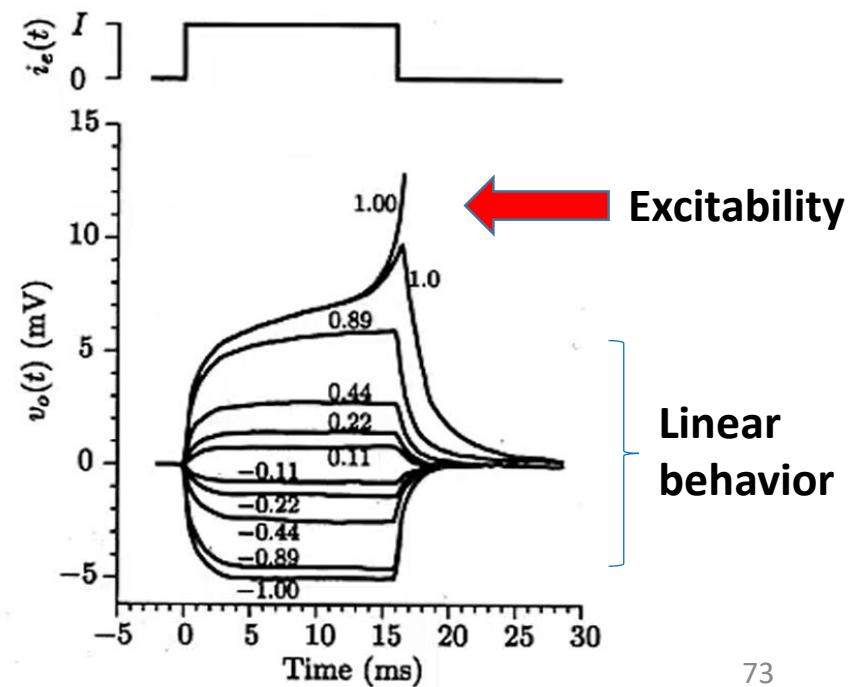
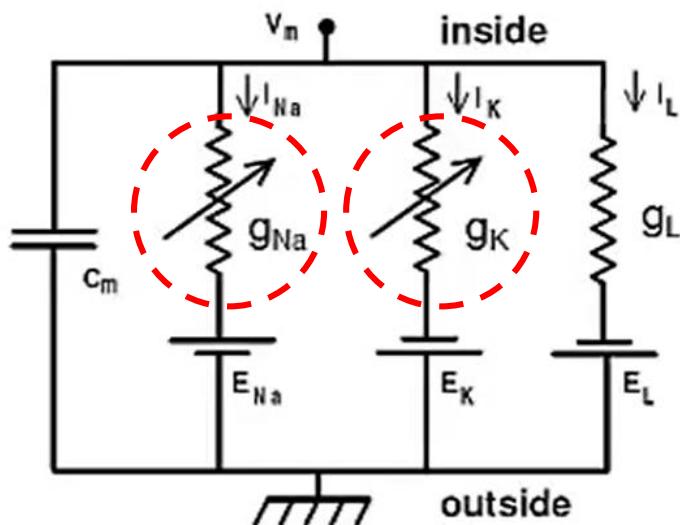
This is how fast it gets there

# Anatomy of A Spike

A to ymotsA

# Equivalent Circuit Model

- The variable conductances associated with the ion channels make the model much more interesting
- This is due to the nonlinearities of the ion channel conductances



# Dynamics of Activation and Deactivation

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- Conductances of the channels:

$$g_K(V) = \overline{g_K} n^4$$

$$g_{Na}(V) = \overline{g_{Na}} m^3 h$$

$\overline{g_K}$  and  $\overline{g_{Na}}$  are the total (maximum) conductances of the channels

are thus **voltage dependent**

- All  $n$ ,  $m$  and  $h$  values have **time constants** in their dynamic behavior

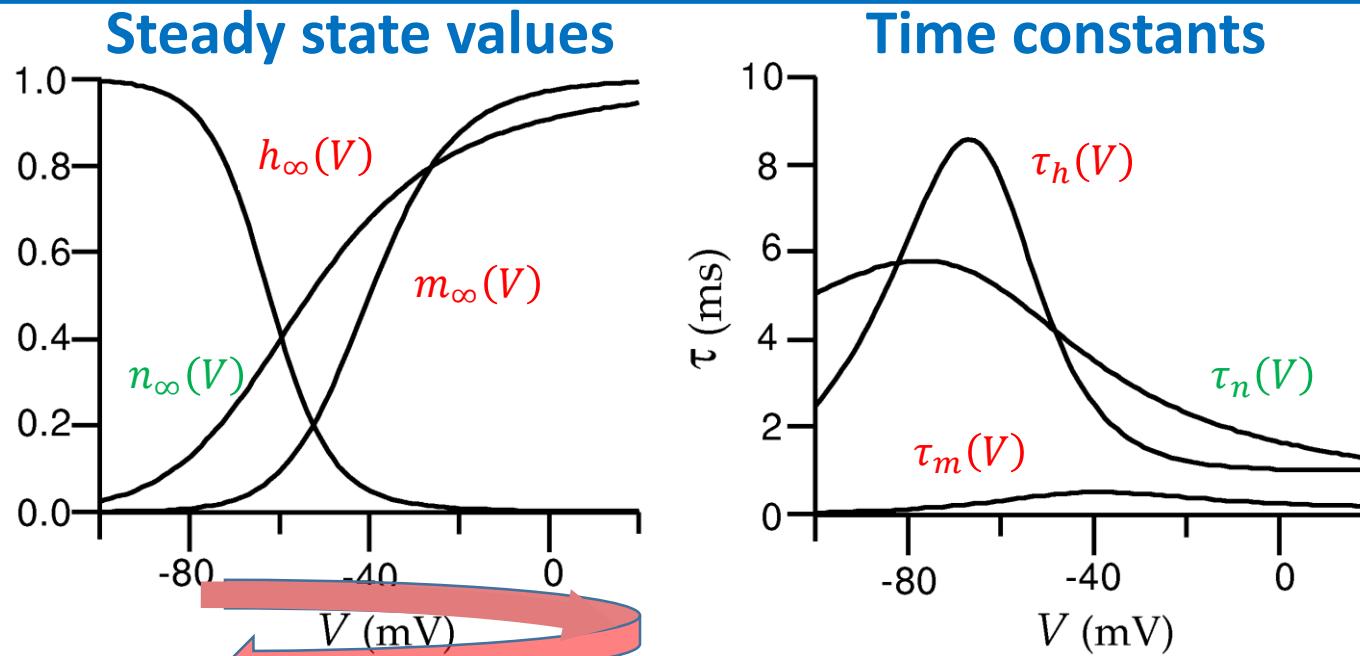
$$\tau_n(V) \frac{dn}{dt} = n_\infty(V) - n$$

$$\tau_m(V) \frac{dm}{dt} = m_\infty(V) - m$$

$$\tau_h(V) \frac{dh}{dt} = h_\infty(V) - h$$

→ This causes the channel conductances  $g_K$  and  $g_{Na}$  to also depend on these time dynamics

# Dynamics of Activation and Inactivation



As voltage increases:

Rapid increase  
in voltage and  
then slowing

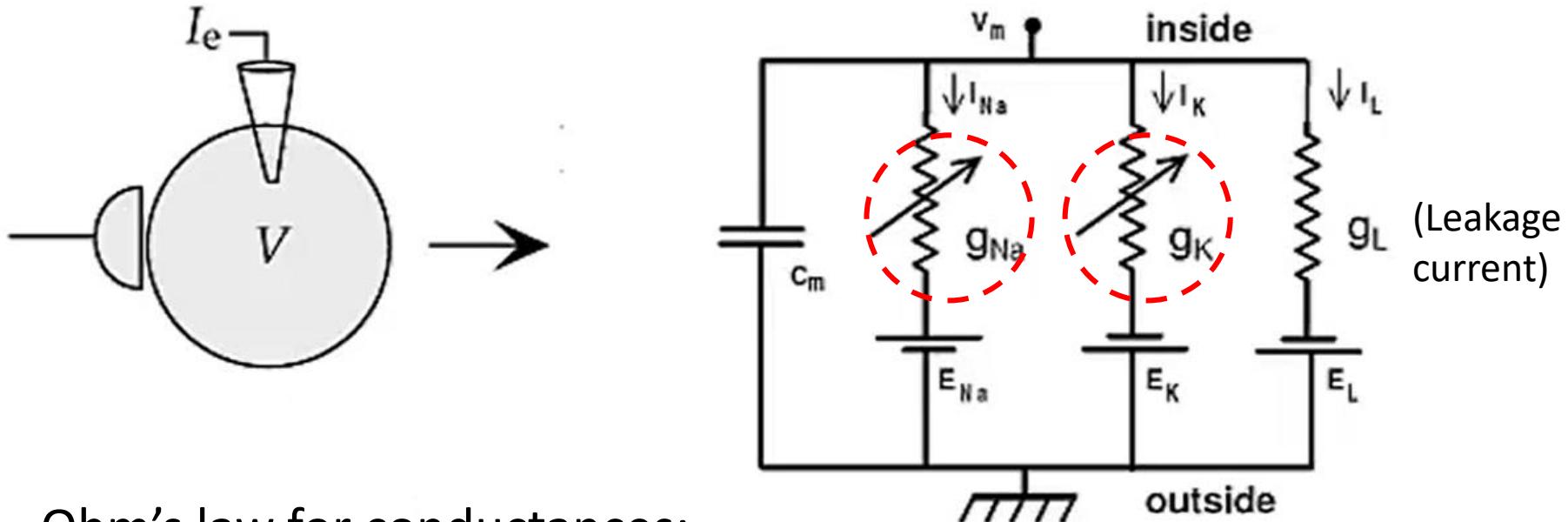
- The sodium channel first opens (a small  $\tau_m$ )  $\rightarrow m_\infty \rightarrow 1$
- But then closes (a larger  $\tau_h$ )  $\rightarrow h_\infty \rightarrow 0$

Decrease in  
voltage towards  
hyperpolarization

- The potassium channel is activated after the opening of the sodium channel ( $\tau_n > \tau_m$ ), and has a higher probability of being open for larger voltages  $\rightarrow n_\infty \rightarrow 1$

75

# Equivalent Circuit Model – Summary



$$V - E_i = R_i I_i \quad \rightarrow \quad I_i = g_i(V - E_i)$$

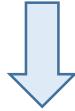
All currents:

$$C_m \frac{dV}{dt} + \sum_i g_i(V - E_i) = I_{ext}$$

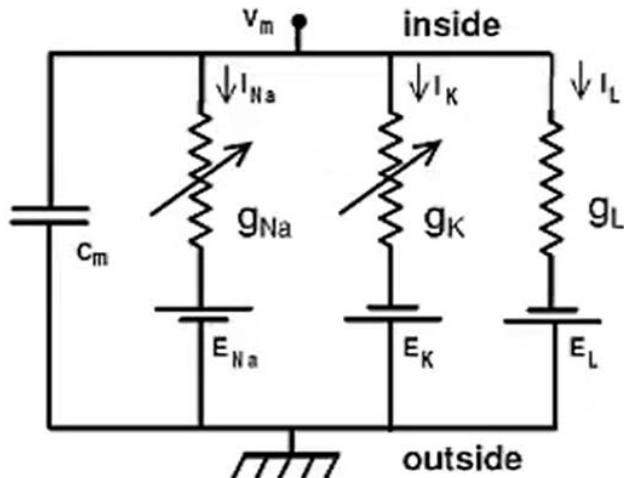
Capacitive current      Ionic currents      Externally applied current

# Hodgkin and Huxley's Nobel Equation

$$C_m \frac{dV}{dt} = - \sum_i g_i(V - E_i) + I_{ext}$$



$$-C_m \frac{dV}{dt} = g_L(V - E_L) + \overline{g_K} n^4(V - E_K) + \overline{g_{Na}} m^3 h(V - E_{Na}) - I_e$$



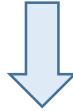
$$\frac{dn}{dt} = \alpha_n(V)(1 - n) - \beta_n(V)n$$

$$\frac{dm}{dt} = \alpha_m(V)(1 - m) - \beta_m(V)m$$

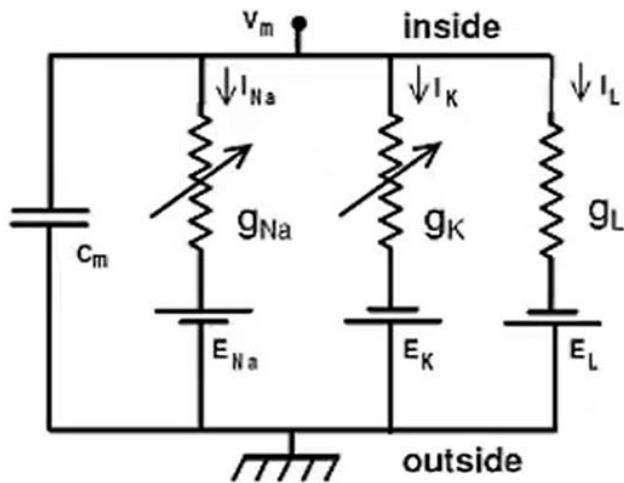
$$\frac{dh}{dt} = \alpha_h(V)(1 - h) - \beta_h(V)h$$

# Hodgkin and Huxley's Nobel Equation

$$C_m \frac{dV}{dt} = - \sum_i g_i(V - E_i) + I_{ext}$$



$$-C_m \frac{dV}{dt} = g_L(V - E_L) + \overline{g_K} n^4(V - E_K) + \overline{g_{Na}} m^3 h(V - E_{Na}) - I_e$$



- The dynamics are explained by a differential equation with 2 nonlinear effects:
  1. Multiplicative factors relating the sub-unit behavior to channel conductances
  2. Voltage dependence of the sub-unit dynamics

# Hodgkin and Huxley's Nobel Equation

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*Studies of spike-generation mechanism in “giant squid axons” won Alan Hodgkin and Andrew Huxley the 1963 Nobel prize in physiology or medicine* 79

# Variants of Hodgkin and Huxley's Equation

$$C_m \frac{dV}{dt} = I_e - g_L(V - E_L) - g_{Na}m^3h \cdot (V - E_{Na}) - g_Kn^4 \cdot (V - E_K)$$

- General form of the Hodgkin-Huxley gate model:

$$I = \bar{g}m^a h^b (V - E)$$

See Izhikevich Sec. 5.1 and 5.1.2

- A variant of the Hodgkin-Huxley equation:

$$C_m \frac{dV}{dt} = I_e - \underbrace{g_L(V - E_L)}_{\text{Leak } I_L} - \underbrace{g_{Na}m_\infty(V) \cdot (V - E_{Na})}_{\text{Instantaneous } I_{Na,p}} - \underbrace{g_Kn \cdot (V - E_K)}_{\text{Slower } I_K}$$

with a second equation modeling the slower potassium channel dynamics:

$$\tau(V) \frac{dn}{dt} = -n + n_\infty(V)$$

- This is called the  $I_{Na,p} + I_K$  (**Persistent Na plus K**) model
  - Persistent current:** No inactivation gate involved (no  $h$  gate) for  $Na$  channel
  - Instantaneous current:** Small time constant  $\tau_m$  (i.e.  $m_\infty(V)$  is reached instantly)

# The Output of a Neuron: Action Potential – Summary

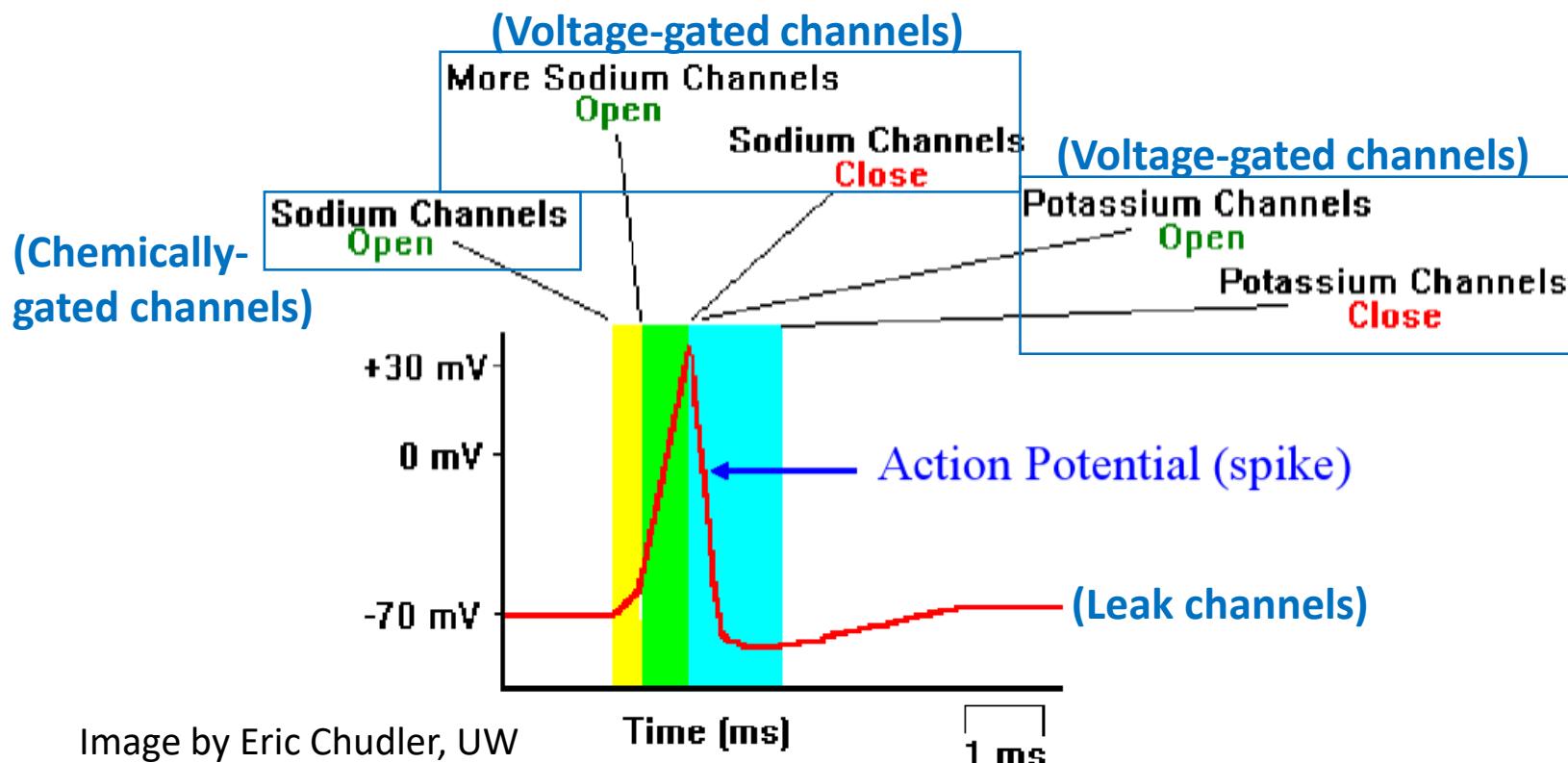
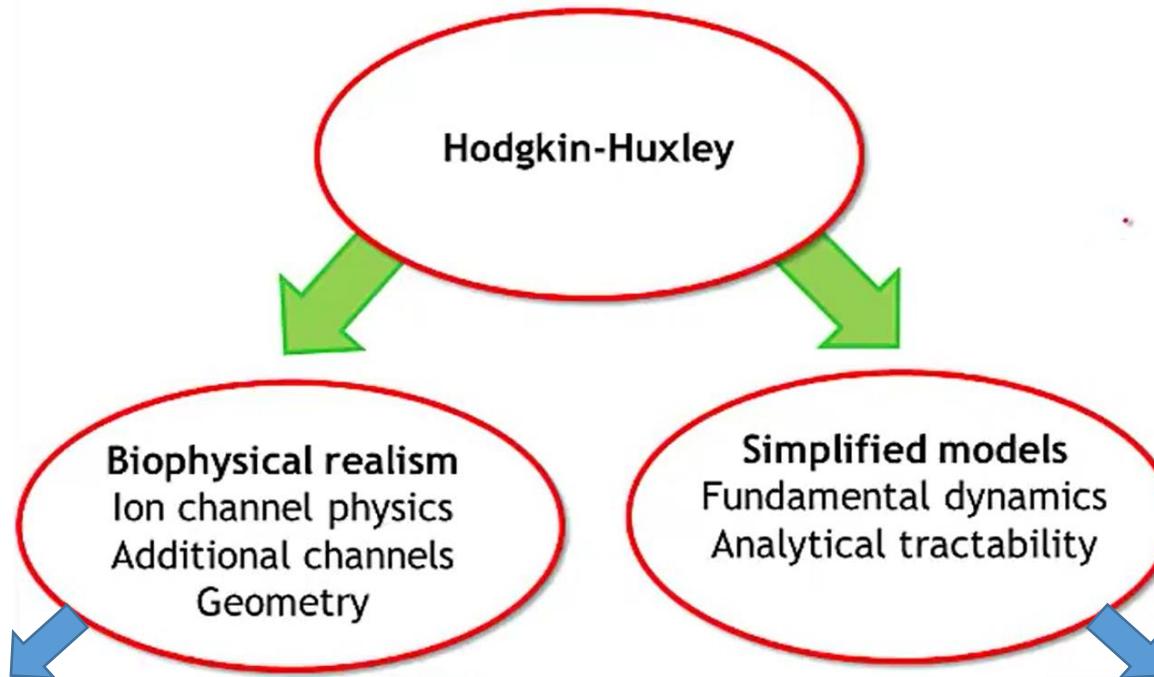


Image by Eric Chudler, UW

# Where To Go As A Modeler?

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- What are the molecular level dynamics of neural activity?
- How do the around 100 different types of channels work?
- A neuron is not just a simple membrane, how does the **geometry** influence the operation of a neuron?
- Can simpler models capture the essence of the neural dynamics?
- Can we have models which can be analyzed mathematically?
- Which may also allow for running large-scale simulations?

# Outline

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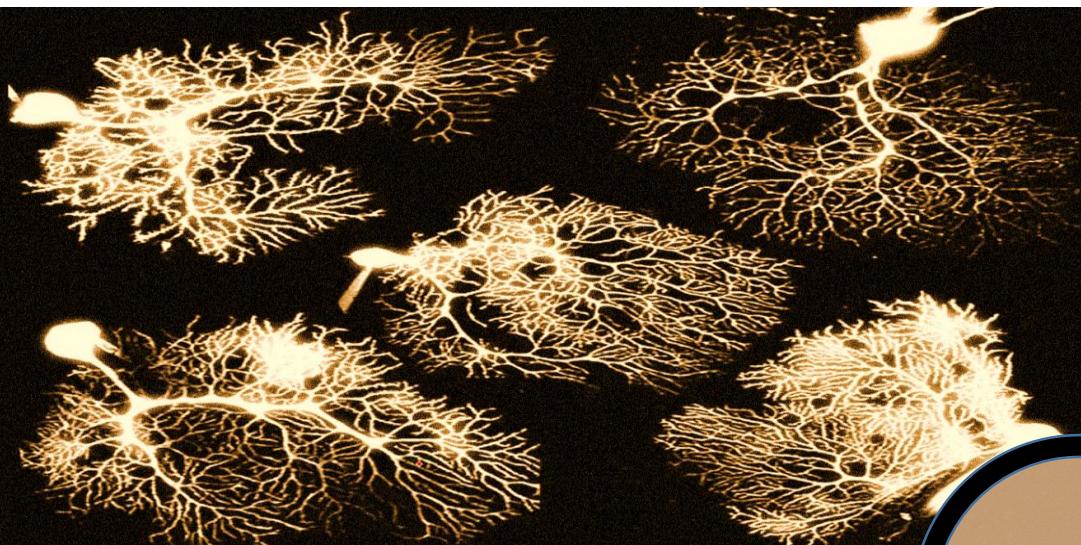
- Sensing & perception
  - Neurons in the brain
  - Visual cortex & receptive fields
  - Vision & perception
- Neurons & spikes
  - Electrical personality of a neuron
  - Ionic channels
  - Action potential
- The Hodgkin-Huxley equation
  - The passive membrane
  - Voltage-gated channels
  - Anatomy of a spike
- Neuronal dynamics
  - Phase portrait models
  - Fixed points and their stability
  - Bifurcation (saddle-node / Hopf)
  - Simplified 2D models

# Next

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## Neuroscience of Learning, Memory, Cognition

### Part I: Neuronal Networks



1

### Neuron Models

Set II

