

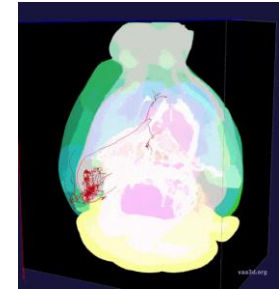
# Neuron and action potential

Computational Neuroscience, Spring 2022

Xu Pan

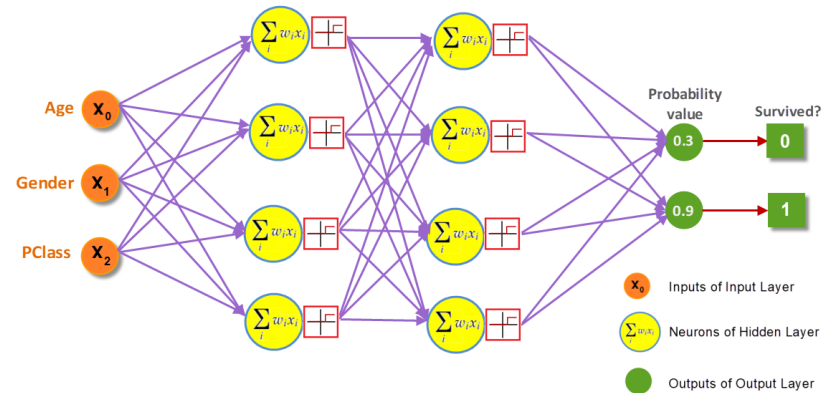
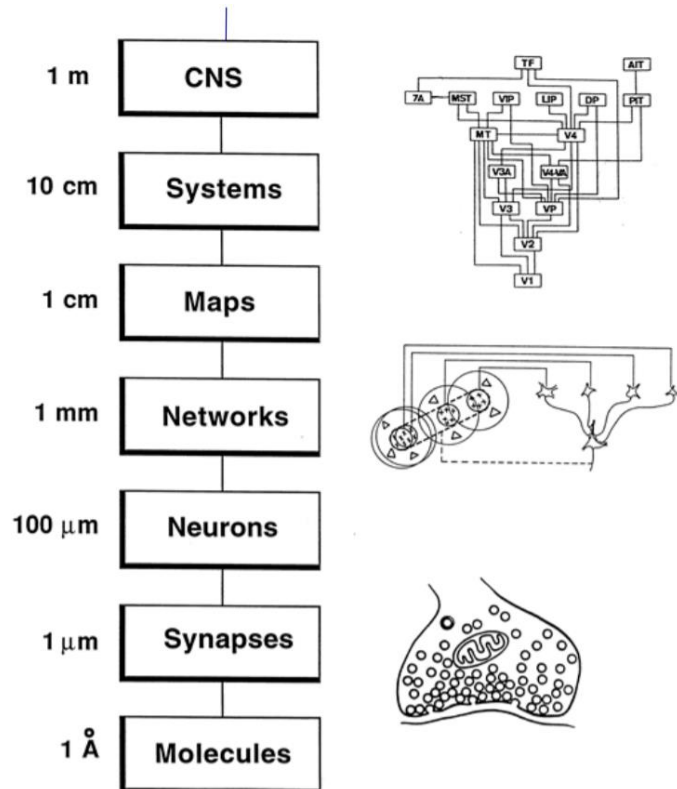
# The Misunderstood Brain

- We know **a lot** about what makes neurons fire.
- We know **a good deal** about wiring patterns.
- We know **only a little** about how information is represented in the neural tissue.
- We know **almost nothing** about how information is processed.
- There is progress every month!



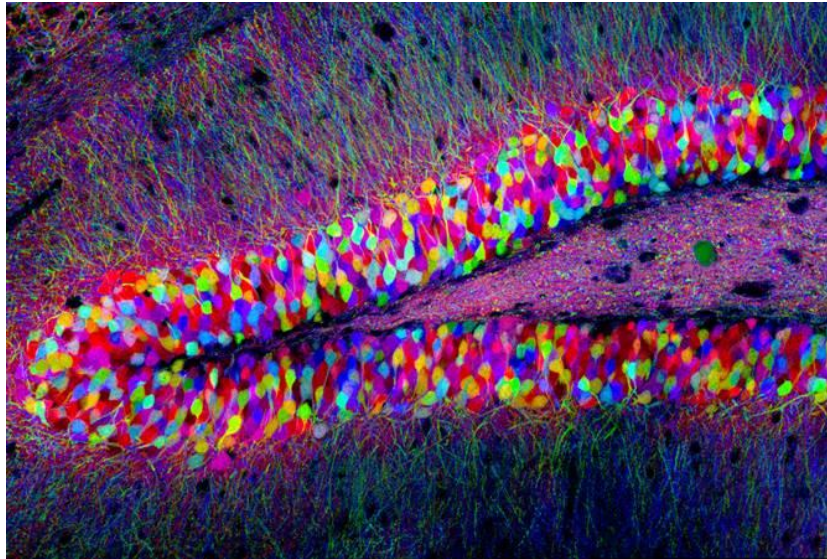
Allen Institute

# Brain v.s. Artificial Neural Networks (again...)



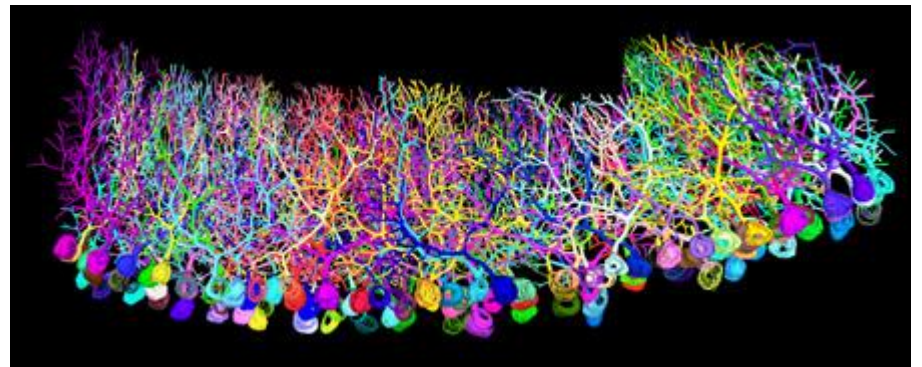
# See some neurons

Hippocampus, CA3,  
Memory formation.



By Tammy Weissman, Harvard University

Cerebellum, Purkinje cells,  
Control motor movement.

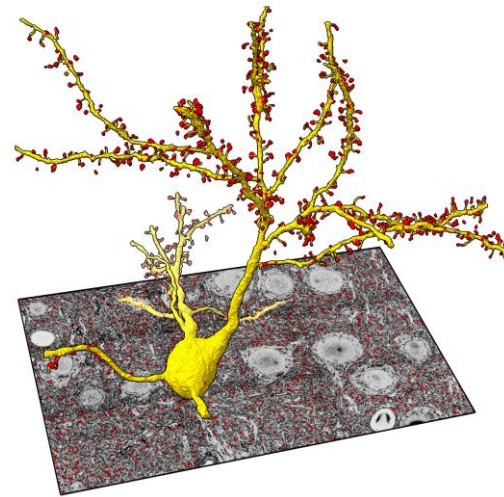
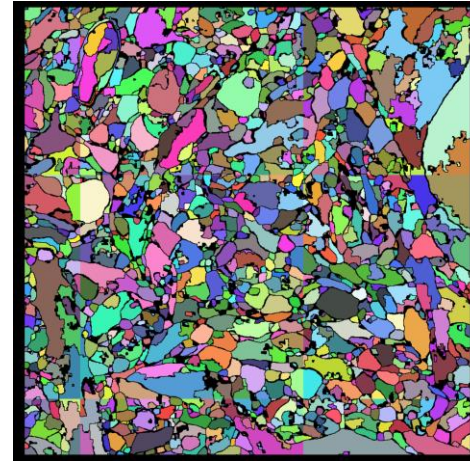
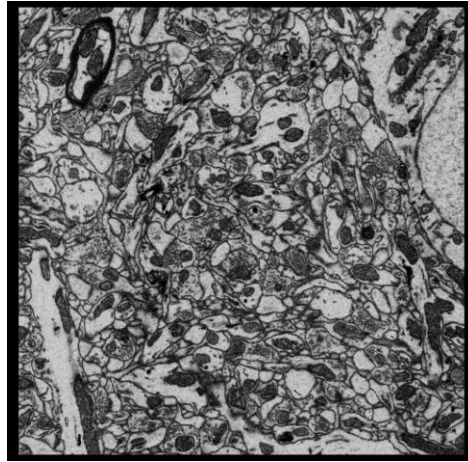


By Hermina Nedelcu

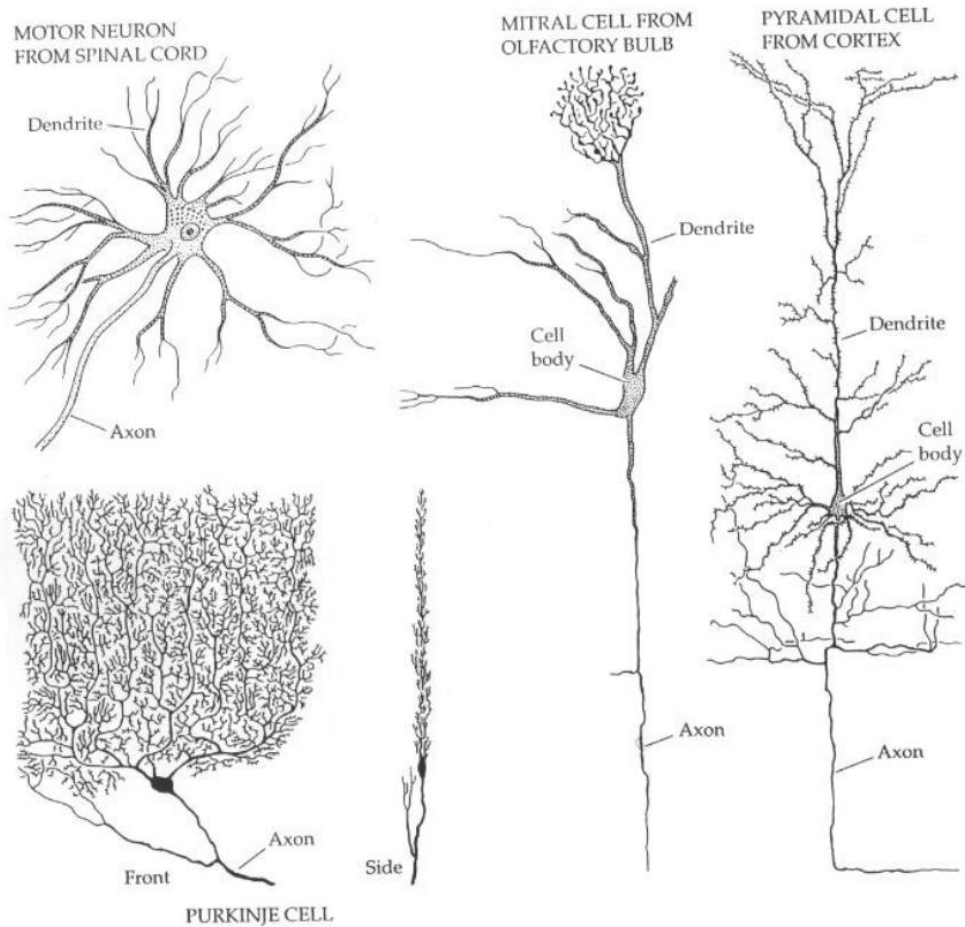
There are so many tools for imaging neurons! Above is Brainbow

# See some neurons

Electron microscopy  
Layer 4 of  
Somatosensory cortex

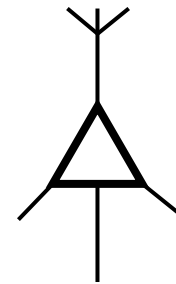
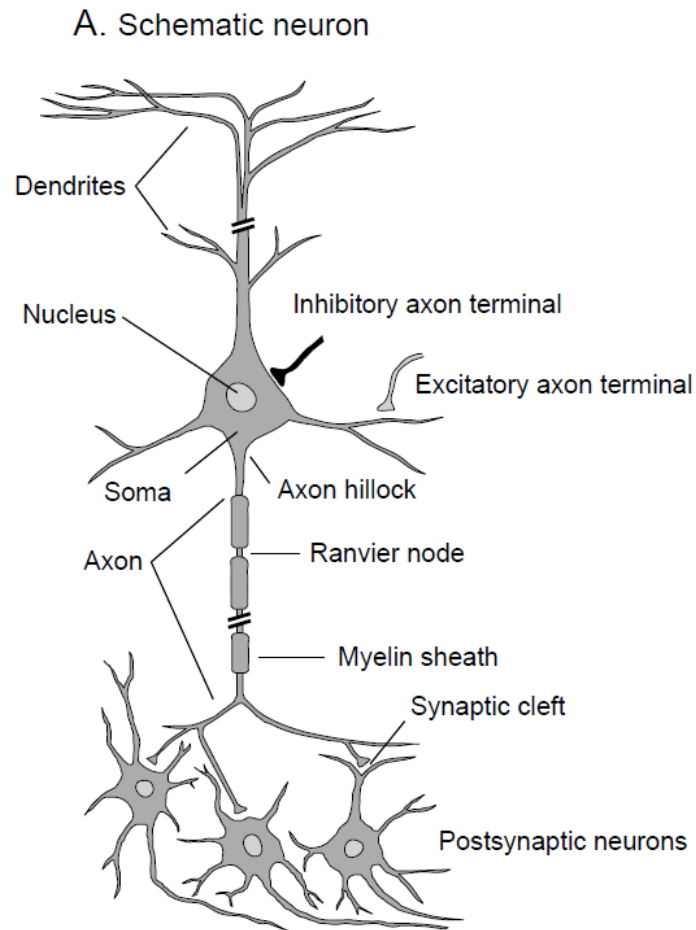


# See some neurons

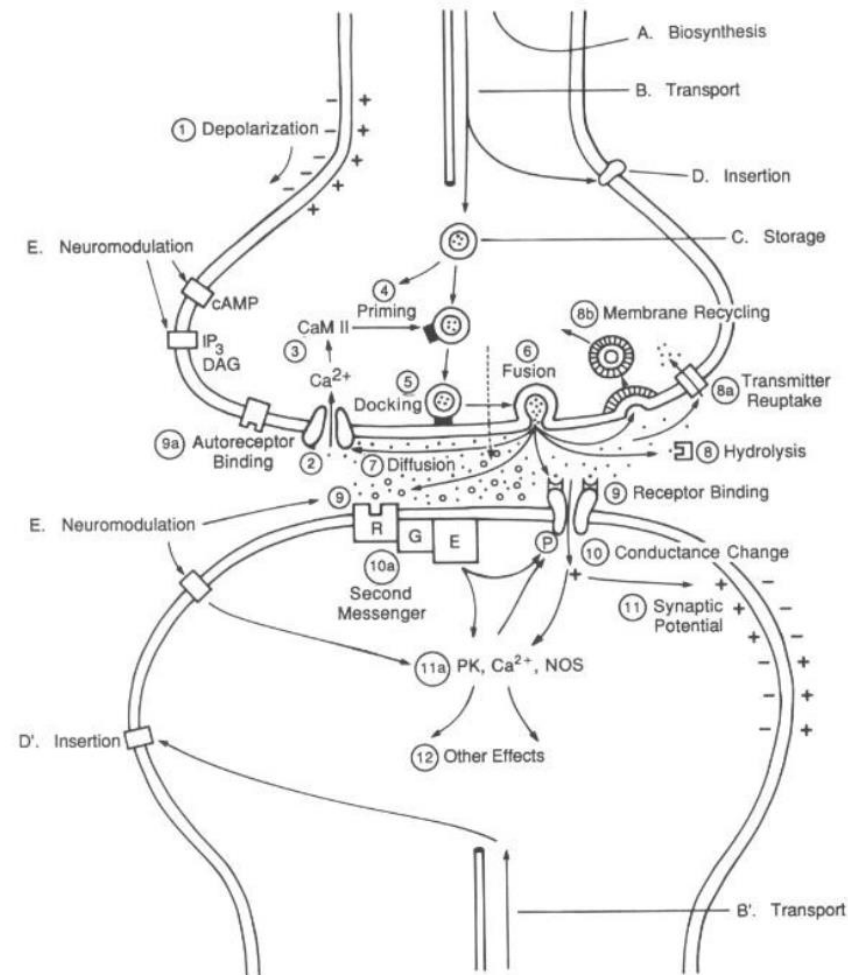




# Neuron



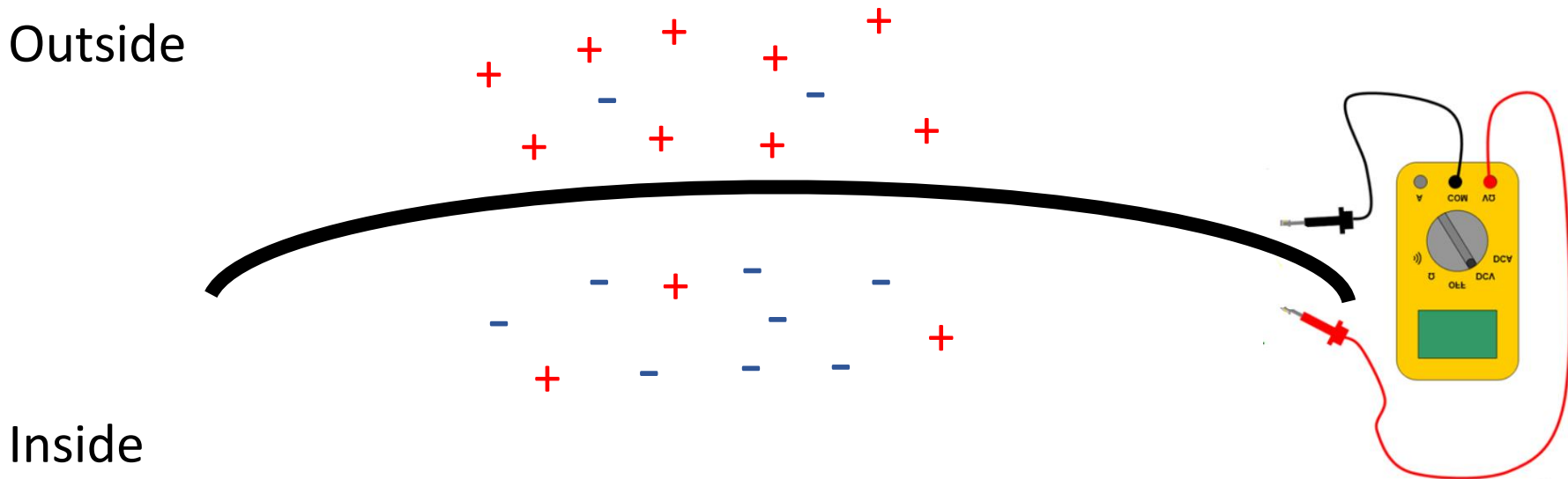
# Synapse





# Membrane potential

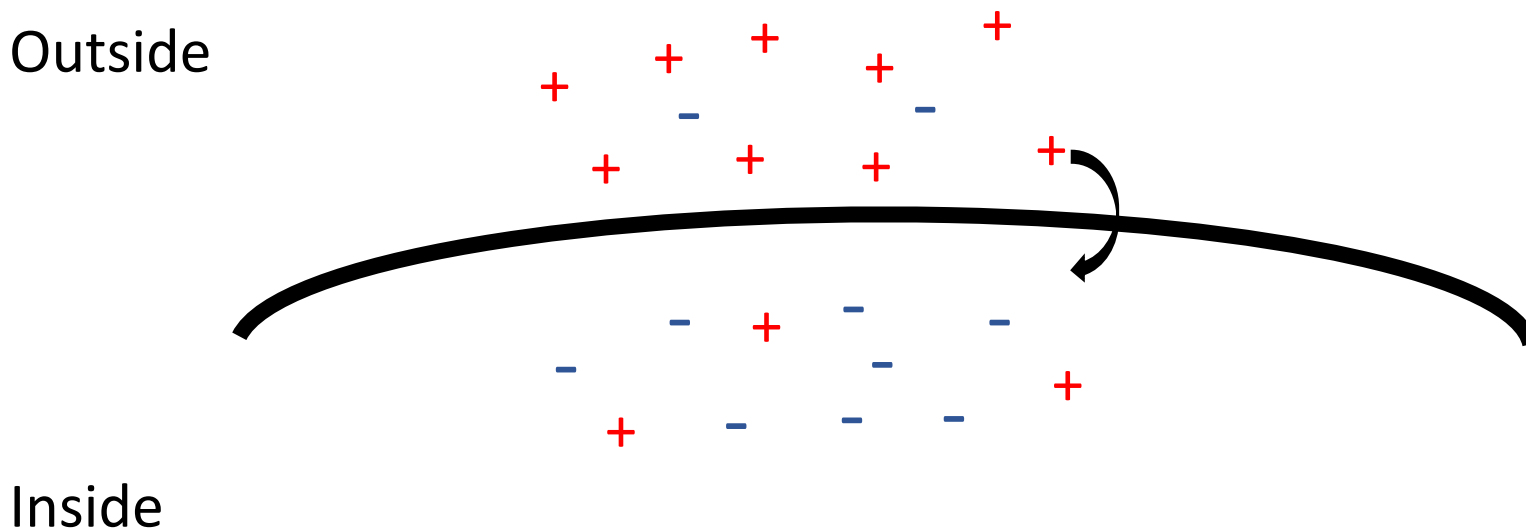
- The more positive ions, the higher potentials.
- Higher potential means more difficult for positive ions to move there.



**Membrane potential  $V_m = V_{in} - V_{out}$**   
**For a typical neuron, this number is -70 mV**

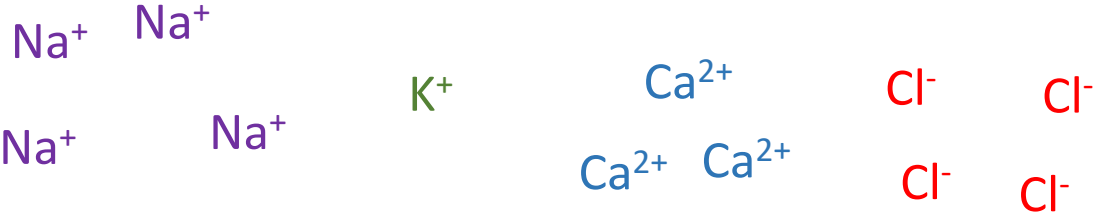
# Depolarize / Hyperpolarize

- Influx of **positive** ions (outflux of **negative** ions) increases  $V_m$ . Depolarize
- Influx of **negative** ions (outflux of **positive** ions) increases  $V_m$ . Hyperpolarize

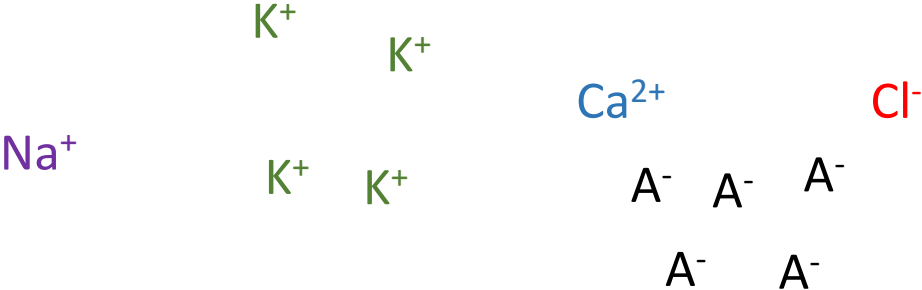


When we talk about current,  $I$ , its direction (sign) is inward.

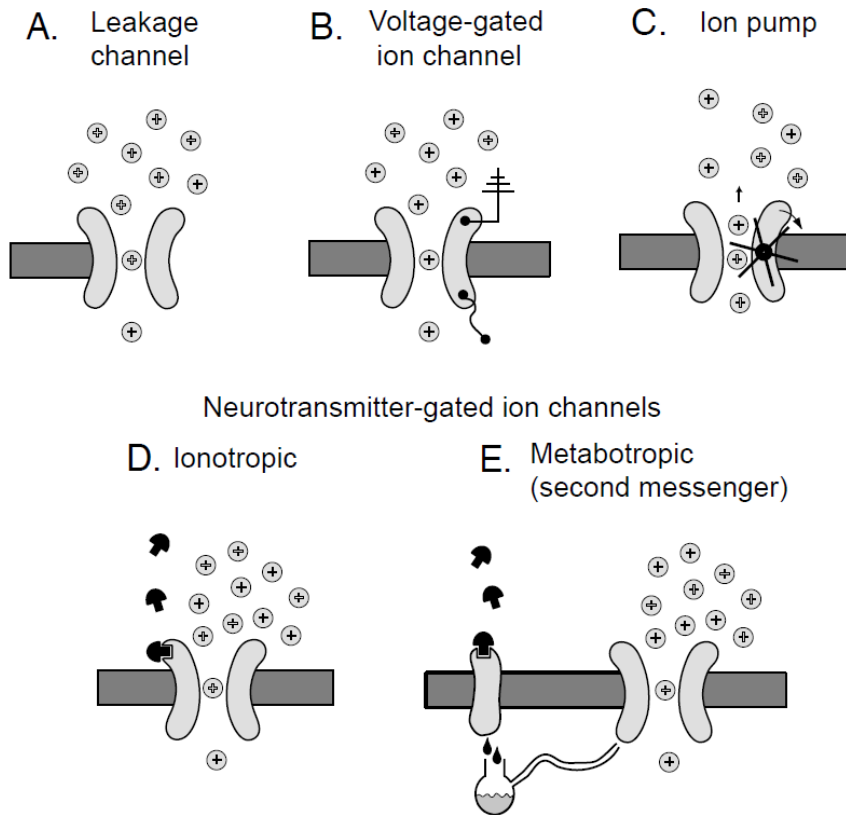
Outside



Inside



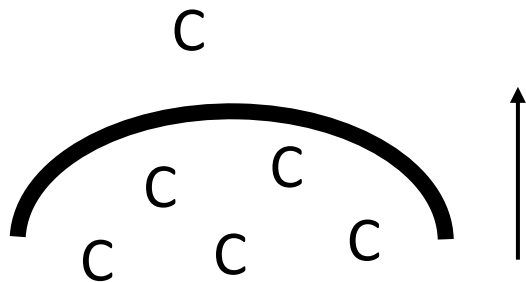
# Ion channels



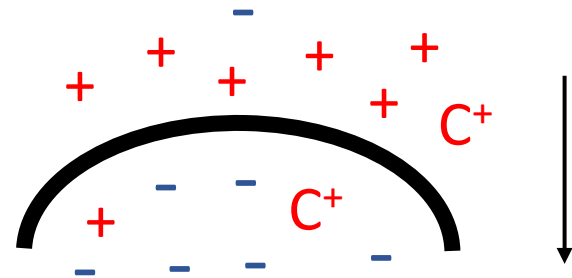
# Nernst equation

- Relationship between  $V_m$ ,  $[C]_{in}$ ,  $[C]_{out}$ .
- There are two passive “forces” that can drive ions across the membrane, i.e. change inside / outside concentrations.

Diffusion “Force”

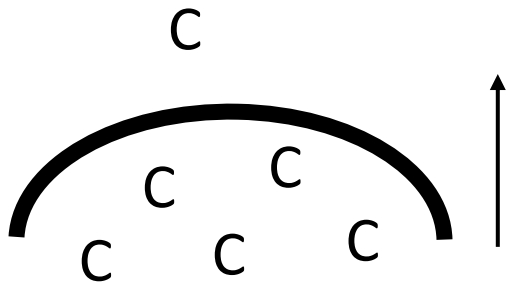


Electric Force



# Nernst equation

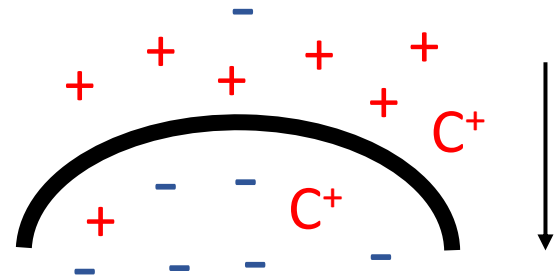
Diffusion “Force”



Fick's law

$$J_{diff} = -D \frac{\partial [C]}{\partial x}$$

Electric Force



Ohm's law

$$J_{drift} = -\mu z [C] \frac{\partial V}{\partial x}$$

$$J_{diff} = J_{drift}$$



$$V_{eq} = -\frac{RT}{zF} \ln \frac{[C]_{in}}{[C]_{out}}$$


# Nernst equation

$$E_c = V_{eq} = -\frac{RT}{zF} \ln \frac{[C]_{in}}{[C]_{out}}$$

This is called *Nernst potential*, *equilibrium potential*, or *reversal potential*.

These 3 numbers are “constant”.

Tiny changes in them lead to drastic changes in  $V_m$ .



Ion	Inside (mM)	Outside (mM)	Equilibrium Potential $E_i = \frac{RT}{zF} \ln \frac{[C]_{out}}{[C]_{in}}$
<b>Mammalian cell</b>			$T = 37^\circ C$
$K^+$	140	5	$62 \log \frac{5}{140} = -89.4mV$
$Na^+$	5-15	145	$62 \log \frac{145}{5-15} = +90 - (+61)mV$
$Cl^-$	4	110	$-62 \log \frac{110}{4} = -89mV$
$Ca^{2+}$	$10^{-4}$	2.5-5	$31 \log \frac{2.5-5}{10^{-4}} = +136 - (+145)mV$



# More about Nernst potential

- If the membrane is only permeable to one type of ion, for example,  $K^+$ .
- Its Nernst potential is eventually where  $V_m$  get to.
- The influx / outflux of  $K^+$  depends on the sign of  $(V_m - E_k)$

$V_m > -89.4 \text{ mV}$ , outflux.

$V_m < -89.4 \text{ mV}$ , influx.

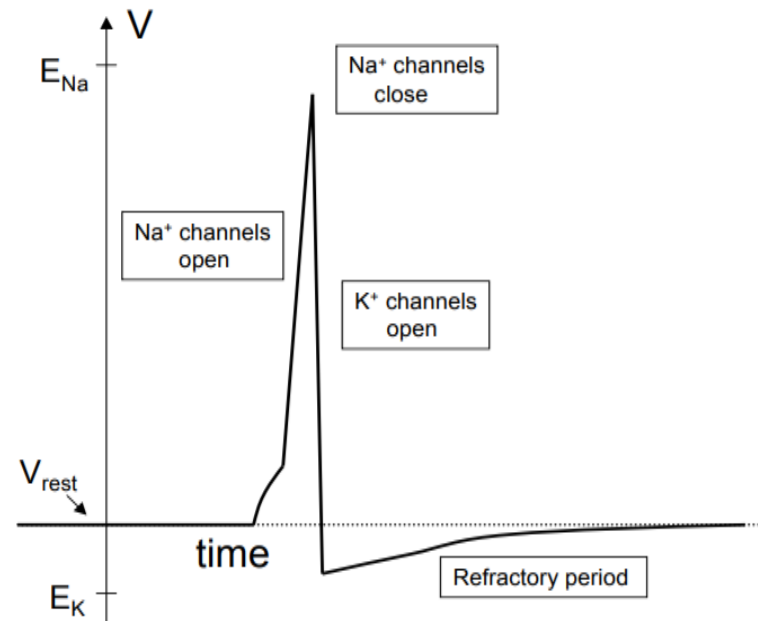
Ion	Inside (mM)	Outside (mM)	Equilibrium Potential $E_i = \frac{RT}{zF} \ln \frac{[C]_{out}}{[C]_{in}}$
$K^+$	140	5	$62 \log \frac{5}{140} = -89.4 \text{ mV}$

# Goldman-Hodgkin-Katz Equation

$$V_m = \frac{RT}{F} \ln \frac{P_K[K^+]_{out} + P_{Na}[Na^+]_{out} + P_{Cl}[Cl^-]_{out}}{P_K[K^+]_{in} + P_{Na}[Na^+]_{in} + P_{Cl}[Cl^-]_{in}}$$

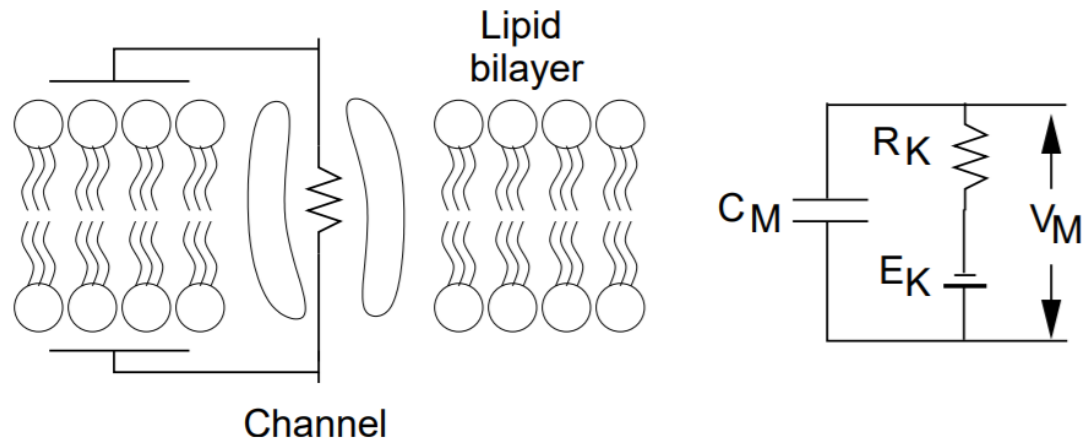
- Similar to Nernst equation, but assume multiple permeable ions.
- Each ion try to bring  $V_m$  to its own Nernst potential. The “strength” is their permeability,  $P$ .
- $P$  is **not** constant and can change according to the state of the neuron. (We will model its dynamics.)

# Goldman-Hodgkin-Katz Equation



Ion	Inside (mM)	Outside (mM)	Equilibrium Potential $E_i = \frac{RT}{zF} \ln \frac{[C]_{out}}{[C]_{in}}$ $T = 37^\circ C$
<b>Mammalian cell</b>			
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# Equivalent circuit model

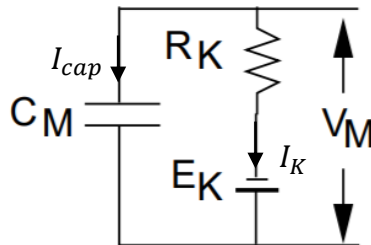


- 1) Resistor represents ion channel permeability
- 2) Battery represents Nernst potential.
- 3) Capacitor represents the ability of the neuron to store charge.

# Equivalent circuit model

- Capacitor can store charge

$$q = C_m V_m \qquad I_{cap} = C_m \frac{dV_m}{dt}$$

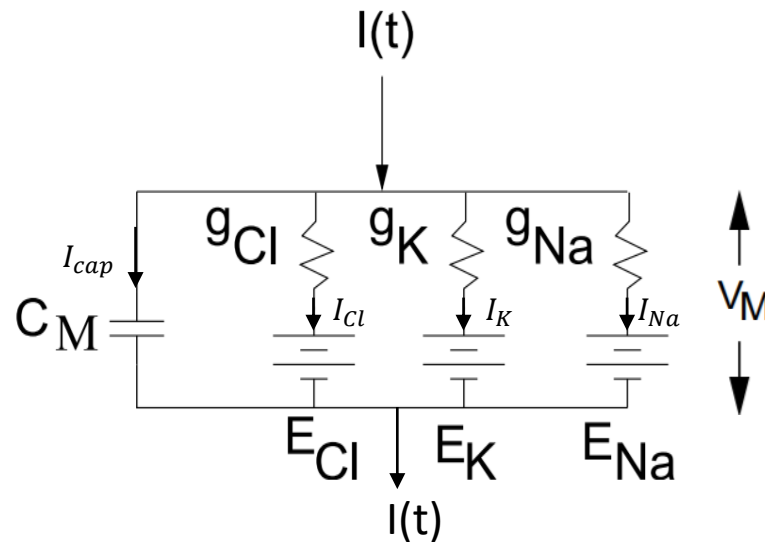


$$I_K = g_K(V_m - E_k)$$

Kirchhoff's Laws  $I_{cap} + I_K = 0$

$$C_m \frac{dV_m}{dt} + g_K(V_m - E_k) = 0$$

# Equivalent circuit model



$$I(t) = I_{cap} + I_K + I_{Cl} + I_{Na}$$

$$C_m \frac{dV_m}{dt} = -g_K(V_m - E_K) - g_{Cl}(V_m - E_{Cl}) - g_{Na}(V_m - E_{Na}) + I(t)$$

# Equivalent circuit model

- Now we can derive how  $V_m$  respond to an input  $I$ .

$$C_m \frac{dV_m}{dt} = -g_K(V_m - E_K) - g_{Cl}(V_m - E_{Cl}) - g_{Na}(V_m - E_{Na}) + I(t)$$

$$C_m \frac{dV_m}{dt} = -g_m(V_m - E_m) + I(t)$$

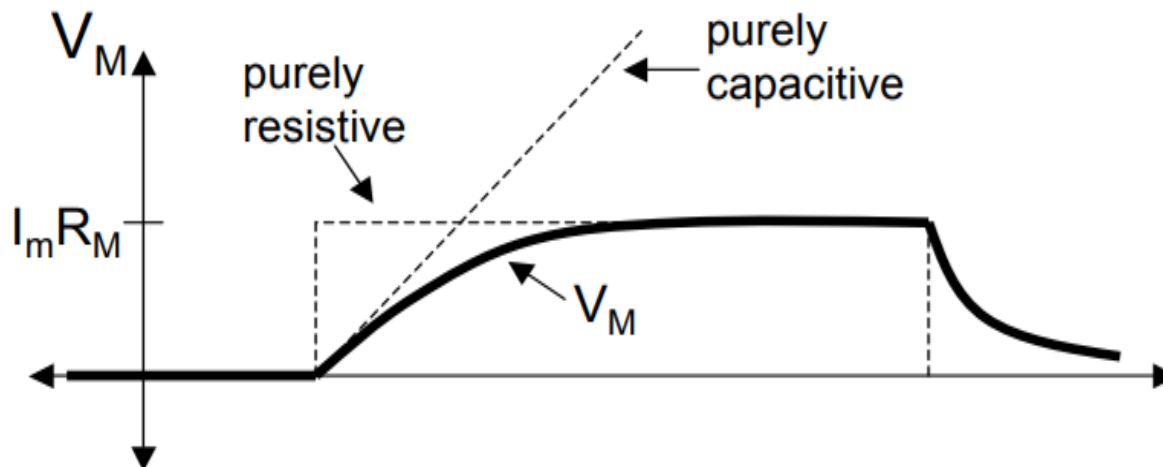
$$I(t) = \begin{cases} I_0 & \text{if } 0 < t < T \\ 0 & \text{otherwise} \end{cases}$$

$$V_m = \begin{cases} \frac{I_0}{g_m} \left(1 - e^{-\frac{t}{\tau_m}}\right) & \text{if } 0 < t < T \\ V_m(T) e^{-t/\tau_m} & \text{otherwise} \end{cases} \quad \tau_m \equiv C_m/g_m$$



# Equivalent circuit model

$$V_m = \begin{cases} \frac{I_0}{g_m} \left(1 - e^{-\frac{t}{\tau_m}}\right) & \text{if } 0 < t < T \\ V_m(T) e^{-t/\tau_m} & \text{otherwise} \end{cases} \quad \tau_m \equiv C_m/g_m$$



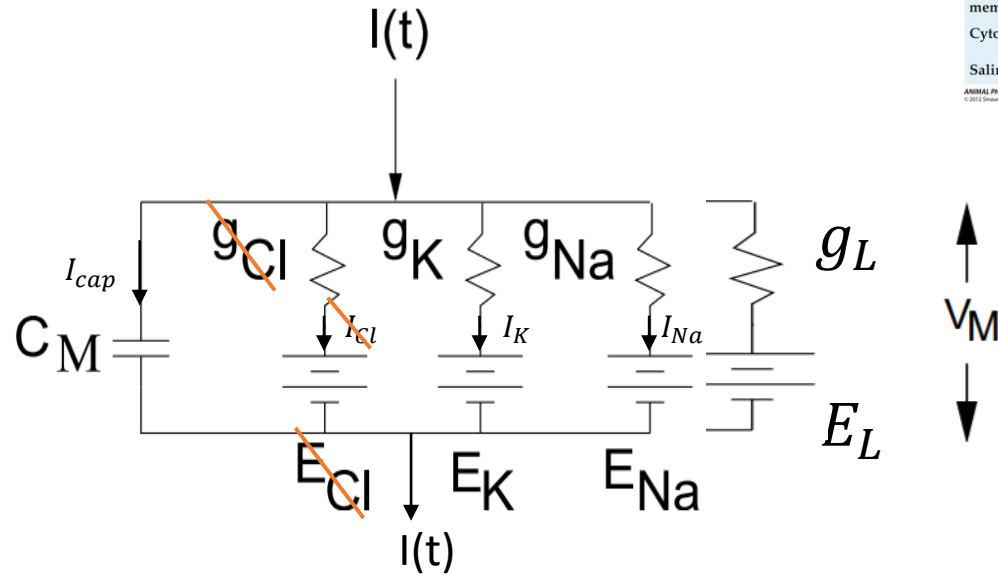
# Hodgkin-Huxley model

Now we have good knowledge about a passive neuron whose  $g_K$  and  $g_{Na}$  are constant.

But this neuron cannot not generate spikes. It only follows the input,  $I(t)$ , with a delay.

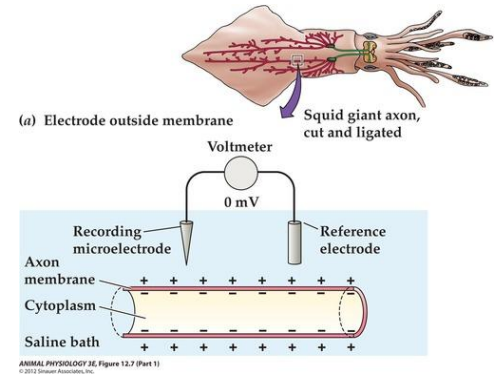
Let's look at how  $g_K$  and  $g_{Na}$  responde to the change of  $V_m$ .

# Hodgkin-Huxley model



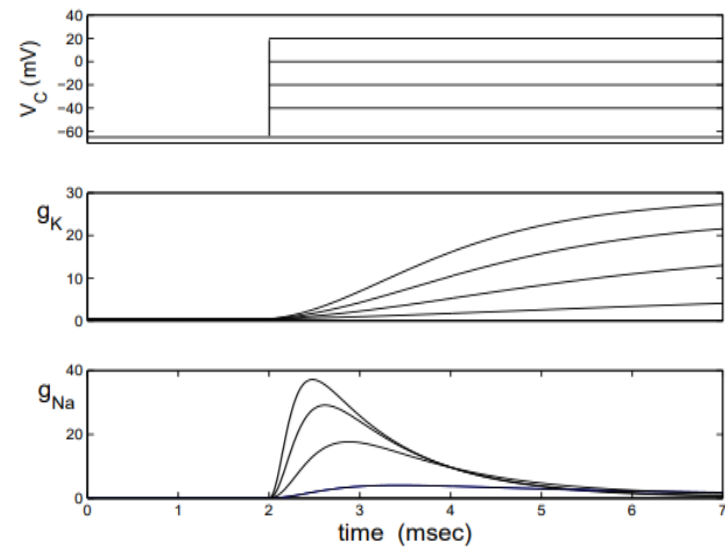
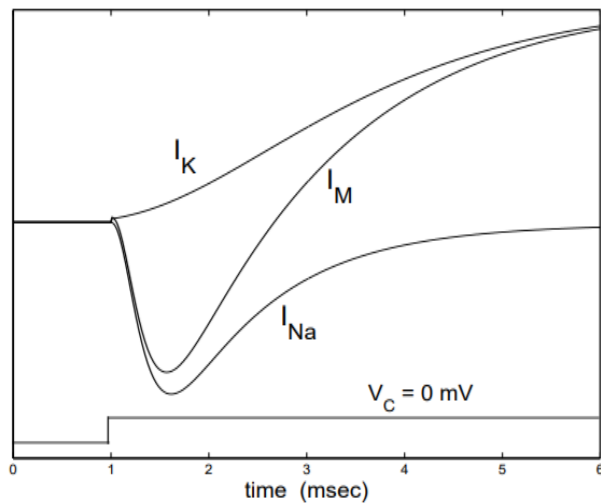
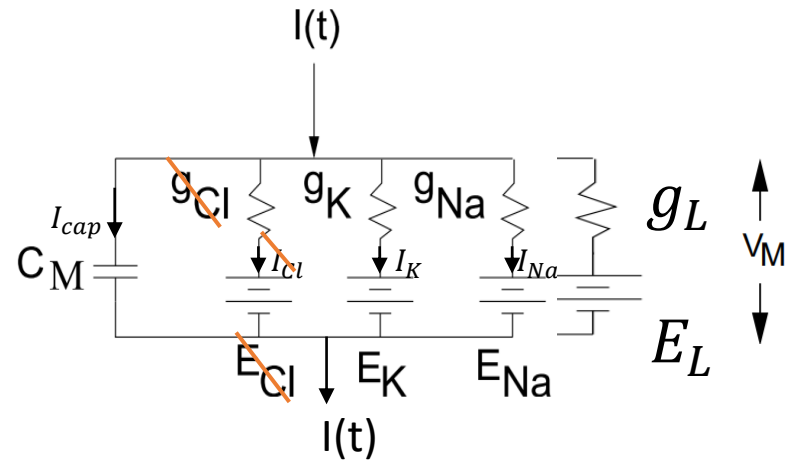
$$g_L = \frac{I_M}{(V_m - E_L)}$$

Measure this by hyperpolarize the neuron (Na and K voltage-gated channels are closed)

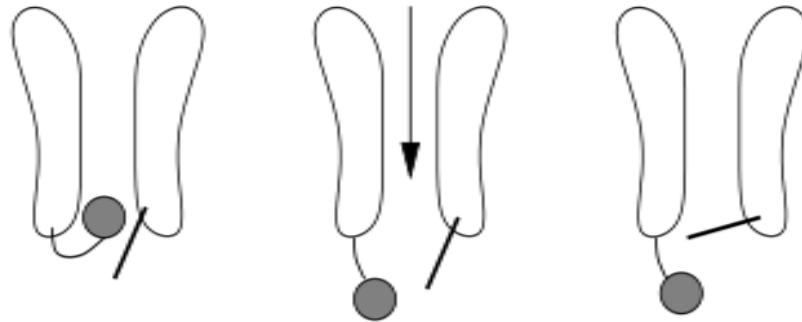


# Hodgkin-Huxley model

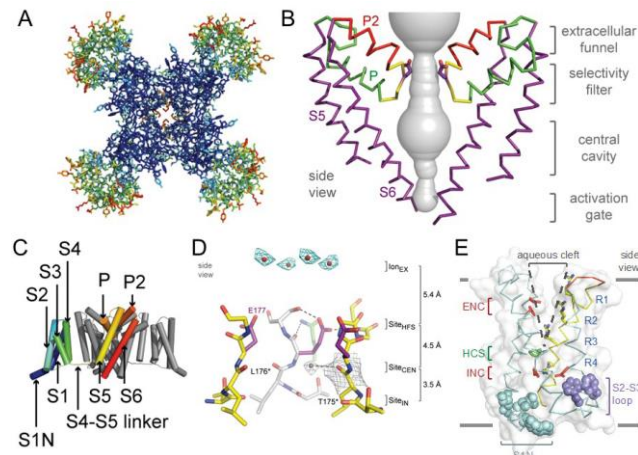
$$g_K(t) = \frac{I_K(t)}{(V_m - E_K)}$$



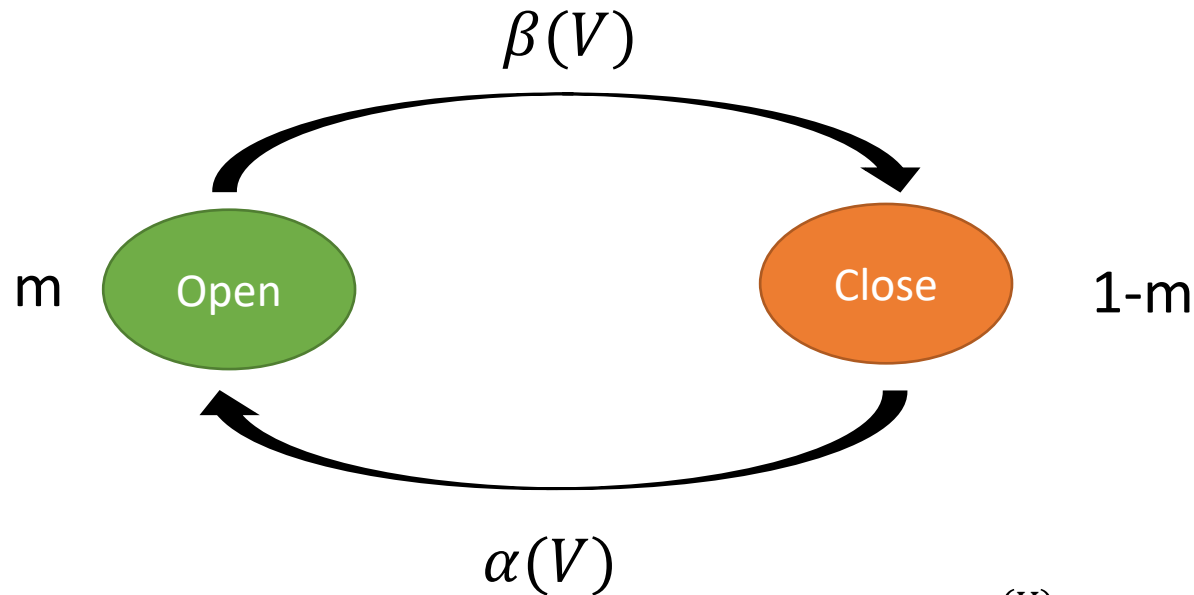
# Hodgkin-Huxley model



## Voltage-gated sodium channel



# Voltage-gated channels



$$m_{\infty}(V) = \frac{\alpha(V)}{\alpha(V) + \beta(V)} \quad \tau(V) = \frac{1}{\alpha(V) + \beta(V)}$$

$$\frac{dm}{dt} = \alpha(V)(1 - m) - \beta(V)m = (m_{\infty}(V) - m)/\tau(V)$$

$$m(t) = m_{\infty}(V) + (m(0) - m_{\infty}(V))e^{-t/\tau(V)}$$

# Hodgkin-Huxley model

$$g_K = \bar{g}_K n^4 \quad \text{and} \quad g_{Na} = \bar{g}_{Na} m^3 h$$

$$\frac{dn}{dt} = \alpha_n(V)(1 - n) - \beta_n(V)n = (n_\infty(V) - n)/\tau_n(V)$$

$$\frac{dm}{dt} = \alpha_m(V)(1 - m) - \beta_m(V)m = (m_\infty(V) - m)/\tau_m(V)$$

$$\frac{dh}{dt} = \alpha_h(V)(1 - h) - \beta_h(V)h = (h_\infty(V) - h)/\tau_h(V)$$

$$C_m \frac{dV_m}{dt} = -g_K(V_m - E_K) - g_{Na}(V_m - E_{Na}) - g_L(V_m - E_L) + I(t)$$



# Hodgkin-Huxley model

$$\bar{g}_K = 120 \text{ mS/cm}^3, \bar{g}_{Na} = 36 \text{ mS/cm}^3, \bar{g}_L = 0.3 \text{ mS/cm}^3, \\ E_{Na} = 50 \text{ mV}, E_K = -77 \text{ mV}, E_L = -54 \text{ mV},$$

$$\alpha_n(V) = 0.01(V + 55)/(1 - \exp(-(V + 55)/10))$$

$$\beta_n(V) = 0.125 \exp(-(V + 65)/80)$$

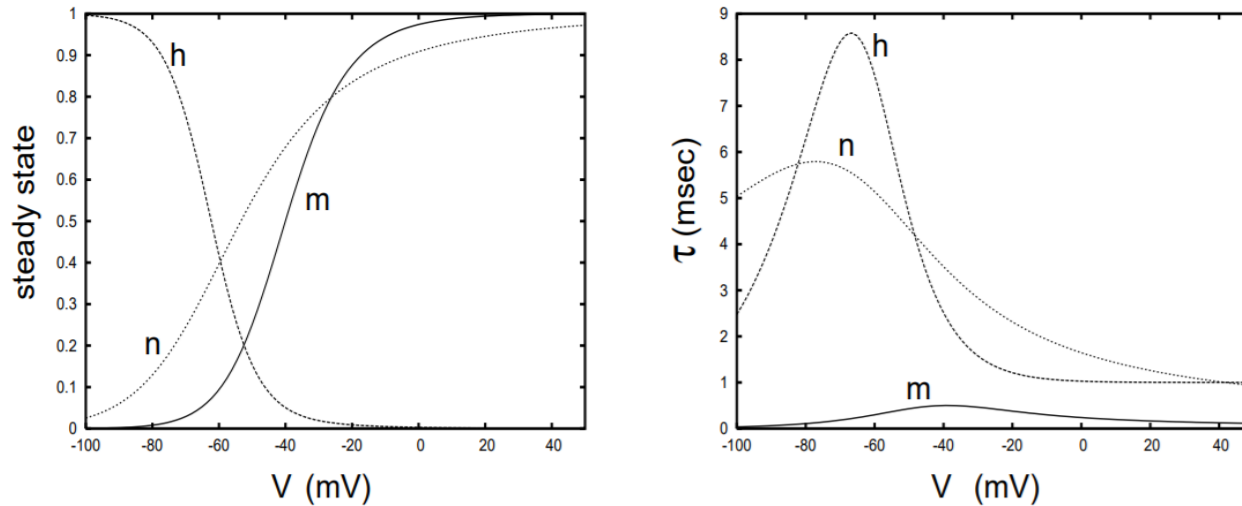
$$\alpha_m(V) = 0.1(V + 40)/(1 - \exp(-(V + 40)/10))$$

$$\beta_m(V) = 4 \exp(-(V + 65)/18)$$

$$\alpha_h(V) = 0.07 \exp(-(V + 65)/20)$$

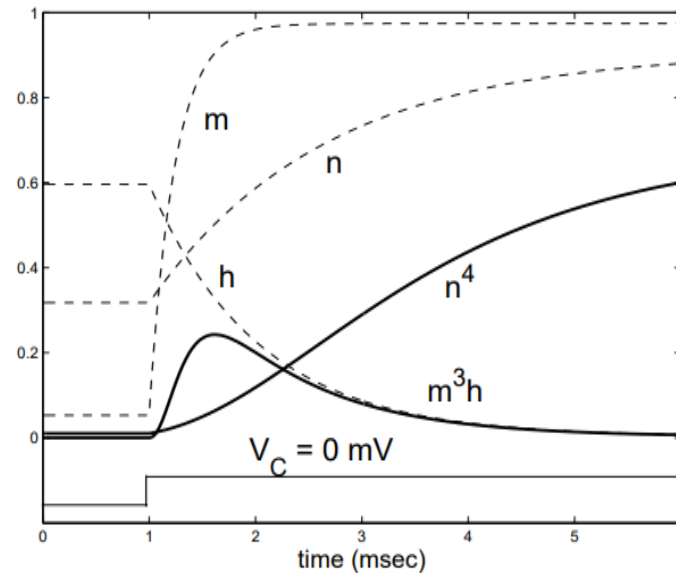
$$\beta_h(V) = 1/(1 + \exp(-(V + 35)/10)).$$

# Hodgkin-Huxley model



$$g_K = \bar{g}_K n^4$$

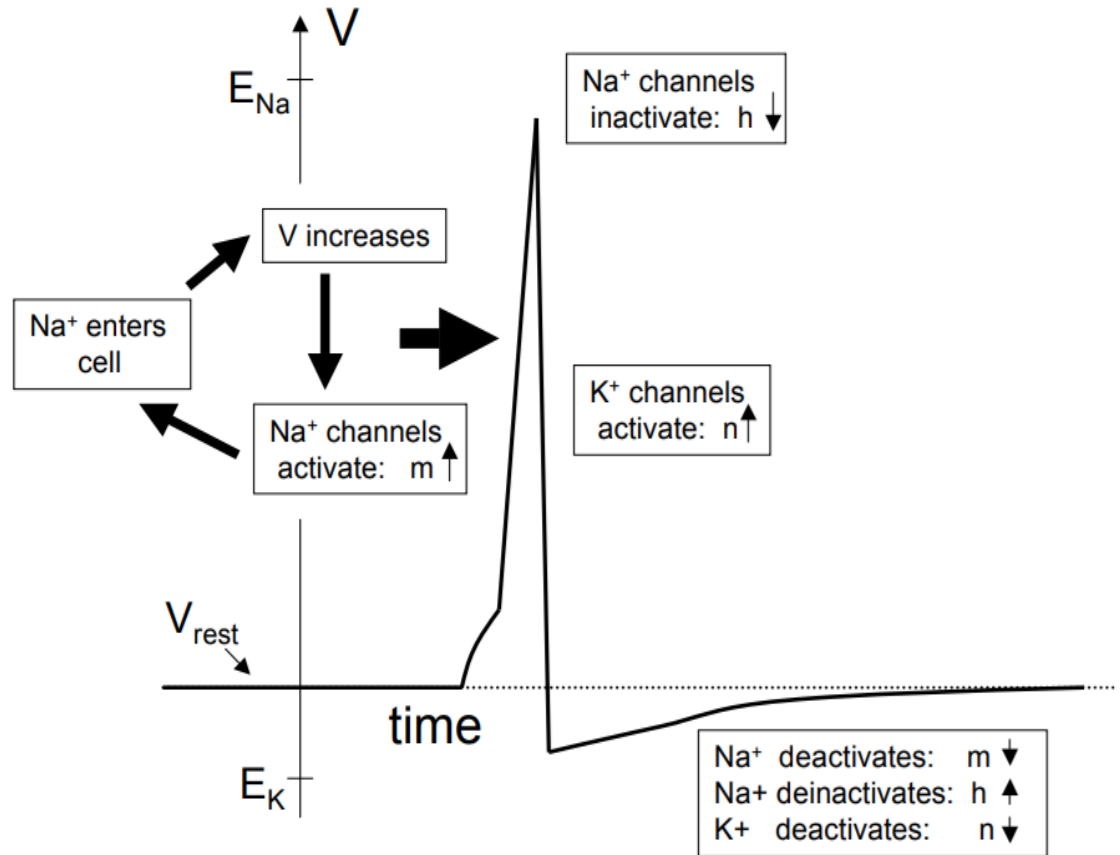
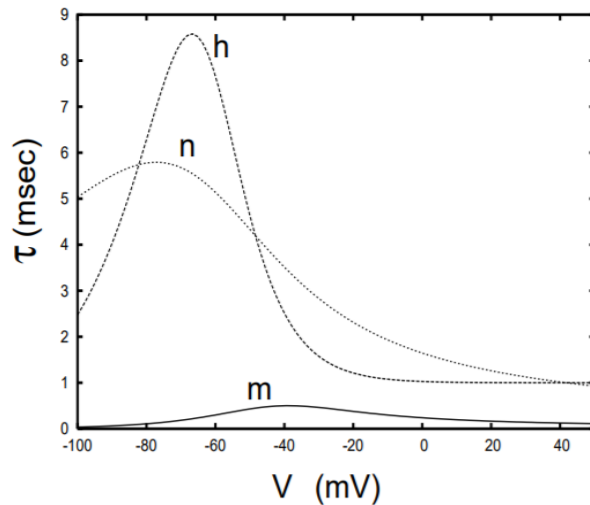
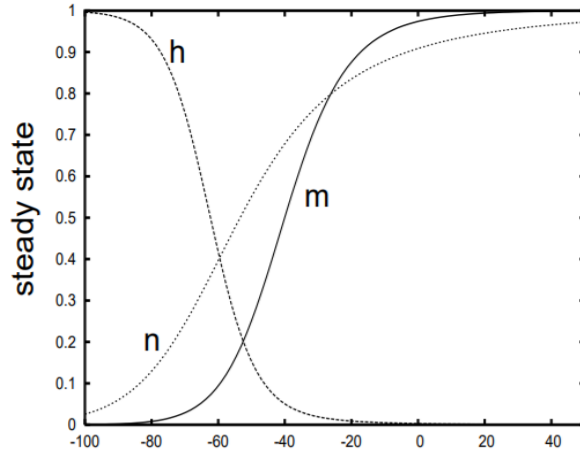
$$g_{Na} = \bar{g}_{Na} m^3 h$$



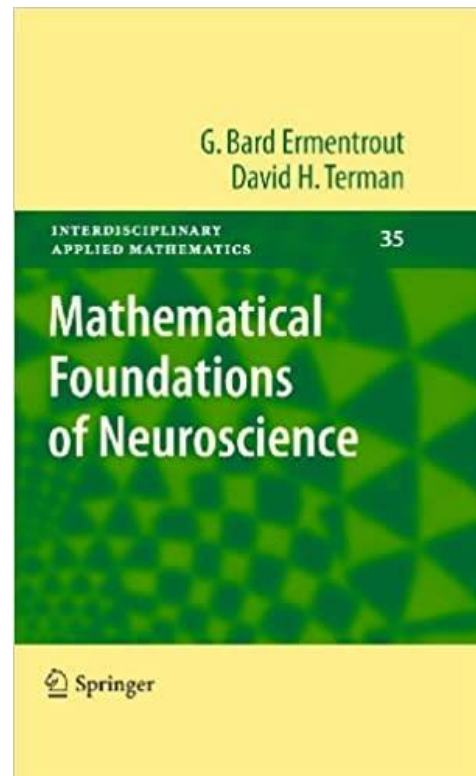
# Hodgkin-Huxley model

$$g_K = \bar{g}_K n^4$$

$$g_{Na} = \bar{g}_{Na} m^3 h$$



# Further reading



## Chapter 1