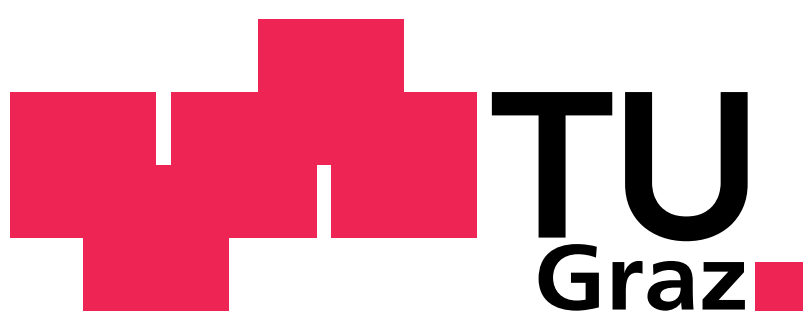


# REAL-TIME INTERACTION WITH AN ELECTROPHYSIOLOGICAL CANCER CELL MODEL

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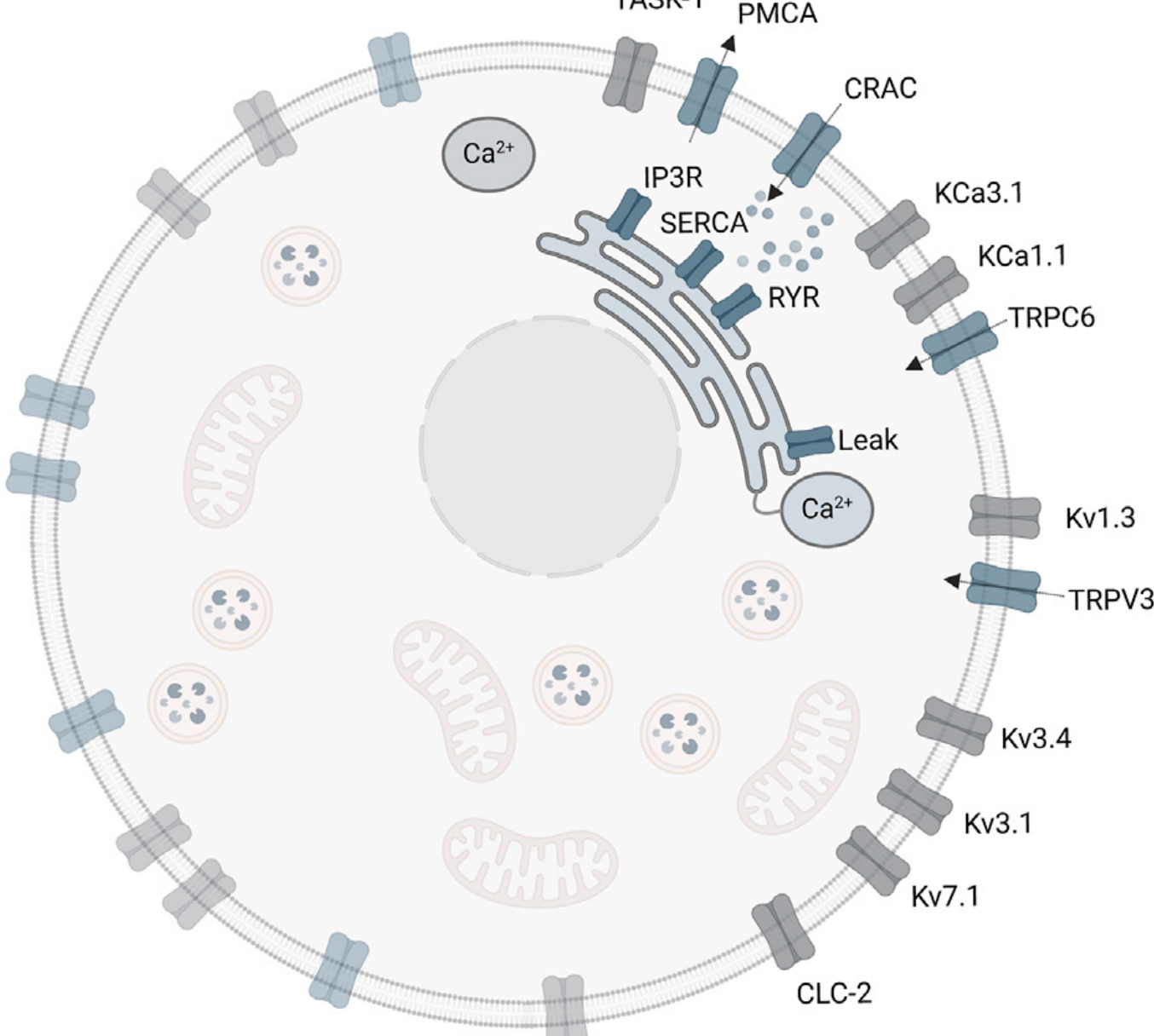
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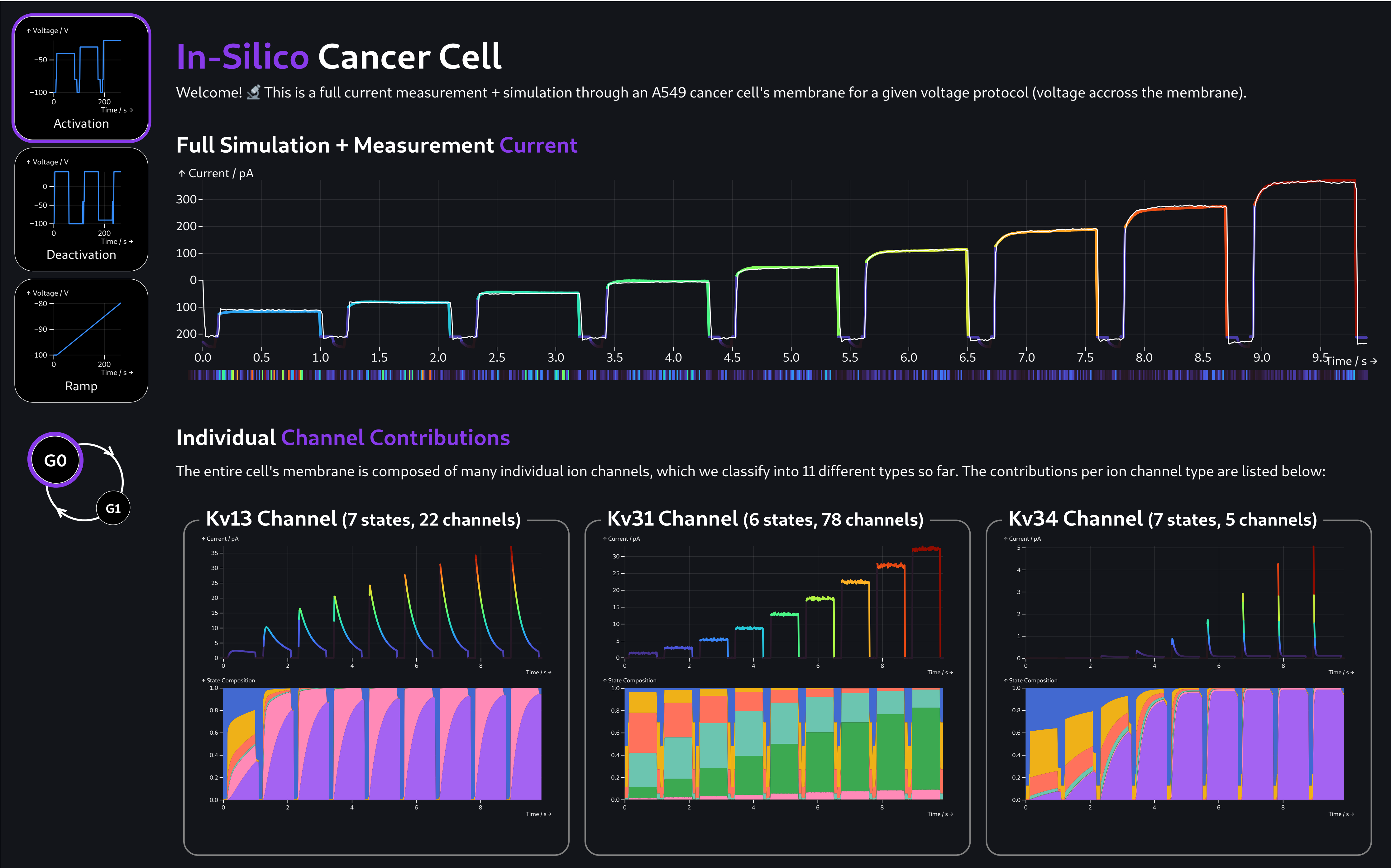
## Introduction

We improve on the A549 electrophysiological cancer cell model introduced in [1, 2], combining numerical methods with an efficient implementation to reduce simulation time to a level where it is feasible for live interaction.



Schematic depiction of a cell, source: [2]. We accelerated the simulation with adaptive timestepping and a highly efficient implementation in the Rust programming language. The corresponding inverse problem is expressed as a quadratic program, solving it within milliseconds. We introduce a visualisation approach of the entire model: a live simulation dashboard available online, running directly in the browser.

## Live, In-Browser Cell Simulation Interface



This interface is available online via [in-silico.hce.tugraz.at](https://in-silico.hce.tugraz.at), try it out!

## Model

The whole cell current  $I : T \rightarrow \mathbb{R}$  over time  $t \in T \subset \mathbb{R}^+$  is the sum of all individual channel contributions  $I_k, k \in \{1, \dots, M\}$  over  $M \in \mathbb{N}$  channel types

$$I(t) := \sum_{k=1}^M N_k I_k(t) = \sum_{k=1}^M N_k g_{k,p_{o,k}}(V(t) - E_k),$$

At each time step, the next state  $\mathbf{s}_{k,n+1} \in [0, 1]^{N_{s,k}}$  of the  $k$ -th channel type is obtained by

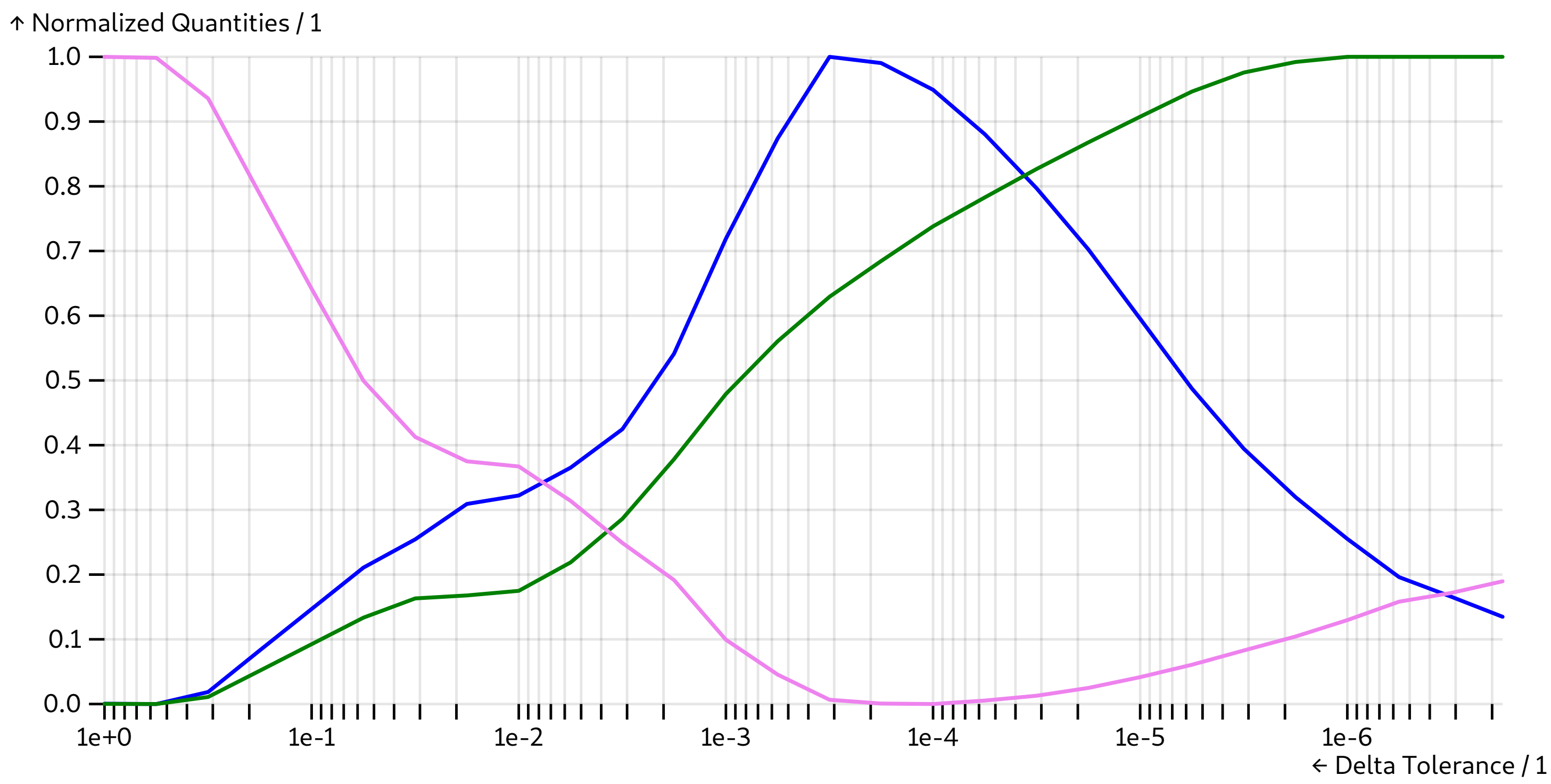
$$\mathbf{s}_{k,n+1} = H_k(V(t_n), \mathbf{C}(t_n), t_n) \mathbf{s}_{k,n}, \quad \text{with} \quad t_n := \sum_{i=0}^n (\Delta t)_i.$$

## Adaptive Timestepping

In order to accelerate the simulation in areas where there is little change to the dynamics, we choose an adaptive step size  $(\Delta t)_n$  based on

$$(\Delta t)_{n+1} = (\Delta t)_n \left( \frac{\Delta^{\text{tol}}}{\sum_{k=1}^M N_k \|\mathbf{s}_{k,n+1} - \mathbf{s}_{k,n}\|_2} \right)^{1/2}.$$

In order to find the optimal  $\Delta^{\text{tol}} \in \mathbb{R}^+$  (the allowed state change in between steps):



Relative change of the average timestep  $\Delta t$  (in blue), simulation runtime (in violet) and step acceptance rate (in green) when varying the delta tolerance  $\Delta^{\text{tol}}$  on a log-scale. All three quantities were normalized from their individual extent to  $[0, 1]$ . The most effective  $\Delta^{\text{tol}}$  is arguably on the order of  $10^{-4}$ .

## Formulation as a Quadratic Program

After simulation of the individual channel currents, we want to find

$$N_{\text{opt}} = \arg \min_{N \in \mathbb{N}_0^M} \frac{1}{2} \|RN - \mathbf{I}_{\text{meas}}\|_2^2.$$

the number of channels per type, with  $\mathbf{I}_{\text{meas}} \in \mathbb{R}^{N_t}$  the experimentally measured current and  $R \in \mathbb{R}^{N_t \times M}$  the matrix of all currents  $I_k$  per channel type. Letting  $\mathbf{d} := \mathbf{I}_{\text{meas}}$  for brevity,

$$N_{\text{opt}} \approx \arg \min_{\mathbf{x} \in \mathbb{R}_+^M} f(\mathbf{x}) = \arg \min_{\mathbf{x} \in \mathbb{R}_+^M} \frac{1}{2} \|\mathbf{R}\mathbf{x} - \mathbf{d}\|_2^2,$$

with cost function  $f : \mathbb{R}^M \rightarrow \mathbb{R}^+$ , which we manipulate to

$$\begin{aligned} f(\mathbf{x}) &= \frac{1}{2} (\mathbf{R}\mathbf{x} - \mathbf{d})^T (\mathbf{R}\mathbf{x} - \mathbf{d}) \\ &= \frac{1}{2} (\mathbf{x}^T \mathbf{R}^T \mathbf{R} \mathbf{x} - \mathbf{x}^T \mathbf{R}^T \mathbf{d} - \mathbf{d}^T \mathbf{R} \mathbf{x} + \mathbf{d}^T \mathbf{d}) \\ &= \frac{1}{2} (\mathbf{x}^T \mathbf{P} \mathbf{x} + \mathbf{x}^T \mathbf{q} + \mathbf{q}^T \mathbf{x}) + \mathcal{O}(1) \\ &= \frac{1}{2} \mathbf{x}^T \mathbf{P} \mathbf{x} + \mathbf{q}^T \mathbf{x} + \mathcal{O}(1) \end{aligned}$$

where we let  $\mathbf{P} := \mathbf{R}^T \mathbf{R} \in \mathbb{R}^{M \times M}$  and  $\mathbf{q} := -\mathbf{R}^T \mathbf{d} \in \mathbb{R}^M$  and leave out the constant  $\mathbf{d}^T \mathbf{d}$  as  $\mathcal{O}(1)$ . We can express the nonnegativity constraint  $\mathbf{x} \geq \mathbf{0}$  as an equality constraint using a slack variable  $\mathbf{s} \in \mathbb{R}_+^M$ ,

$$-\mathbf{x} + \mathbf{s} = \mathbf{0} \quad \Leftrightarrow \quad \mathbf{A}\mathbf{x} + \mathbf{s} = \mathbf{b} \quad \text{with} \quad \mathbf{A} = -\mathbf{I} \in \mathbb{R}^{M \times M} \quad \text{and} \quad \mathbf{b} = \mathbf{0} \in \mathbb{R}^M.$$

This leaves us with a constrained quadratic program,

$$\begin{aligned} \min_{\mathbf{x} \in \mathbb{R}^M} \quad & \frac{1}{2} \mathbf{x}^T \mathbf{P} \mathbf{x} + \mathbf{q}^T \mathbf{x}, \\ \text{s.t.} \quad & \mathbf{A}\mathbf{x} + \mathbf{s} = \mathbf{b}, \quad \mathbf{s} \in \mathbb{R}_+^M. \end{aligned}$$

The integer solution can then be obtained from rounding,

$$N_{\text{opt}} = \lfloor \mathbf{x} \rfloor \in \mathbb{N}_0^M.$$

## Comparison of Optimization Methods

The different approaches were evaluated on the G0 cell cycle phase with the activation voltage protocol. Runtime estimates were obtained on an Intel™i7-5600U CPU.

Algorithm	Abbreviation	Runtime / ms	RMSE / pA
Particle Swarm Optimization	PSO	22571	27.69
Gradient Descent + More Thuente	GD	18924	32.34
Limited-Memory BFGS + Hager Zhang	LBFGS	4845	32.20
Non-Negative Least Squares [3]	NNLS	318	28.00
Quadratic Program	QP	18	28.13

## Conclusion

Efforts to further enhance and complete the first electrophysiological cancer cell model simulation were fruitful, resulting in a new library implementation, an improved inverse problem solution technique and a live in-browser simulation dashboard. Numerically, the stability of the simulation varies greatly with the time step state change tolerance  $\Delta^{\text{tol}}$ , this could be improved using a higher-order integration scheme. There are also many ideas for further customizations that would improve the live simulation dashboard, opening up future usage perspectives.

## References

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