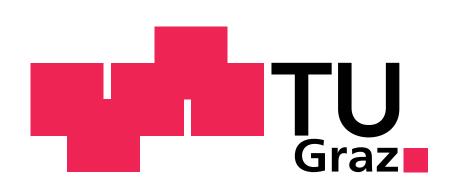
REAL-TIME INTERACTION WITH AN ELECTROPHYSIOLOGICAL CANCER CELL MODEL



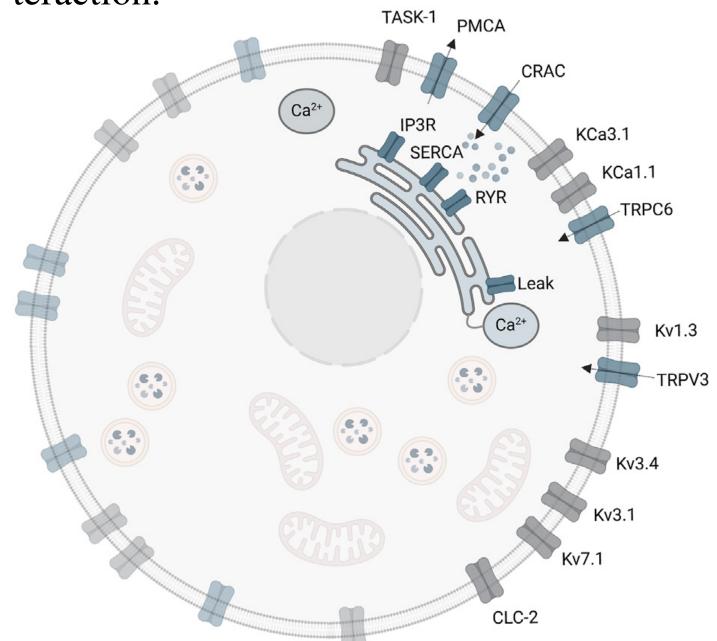
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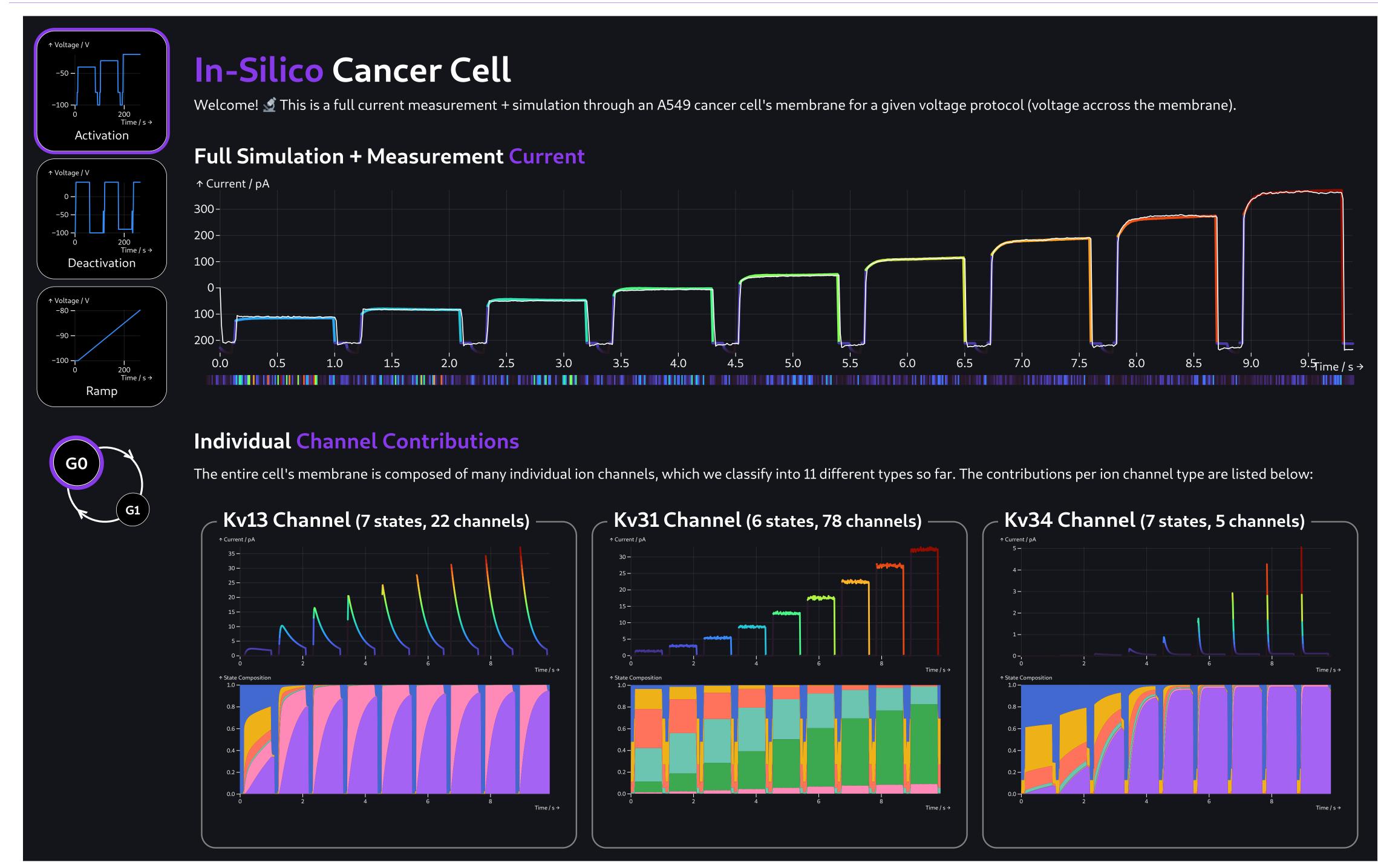
Introduction

We improve on the A549 electrophysiological cancer cell model introduced in [1, 2], combining numerical methods with an efficient implementation to reduce simulation time to a level where it is feasible for live interaction.



Schematic depiction of the cell, source: [2] We accelerated the simulation with adaptive timestepping and a highly efficient implementation in the Rust programming language. The corresponding inverse problem is expressed as a quadratic program, solving it within milliseconds. We introduce a visualisation approach of the entire model: a live simulation dashboard available online, running directly in the browser.

LIVE, IN-BROWSER CELL SIMULATION INTERFACE



This interface is available online via in-silico.hce.tugraz.at, try it out!

Model

The whole cell current $I: T \to \mathbb{R}$ over time $t \in T \subset \mathbb{R}^+$ is the sum of all individual channel contributions $I_k, k \in \{1, ..., M\}$ over $M \in \mathbb{N}$ channel types

$$I(t) := \sum_{k=1}^{M} N_k I_k(t) = \sum_{k=1}^{M} N_k g_k p_{o,k} \left(V(t) - E_k \right).$$

At each time step, the next state $s_{k,n+1} \in [0,1]^{N_{s,k}}$ of the k-th channel type is obtained by

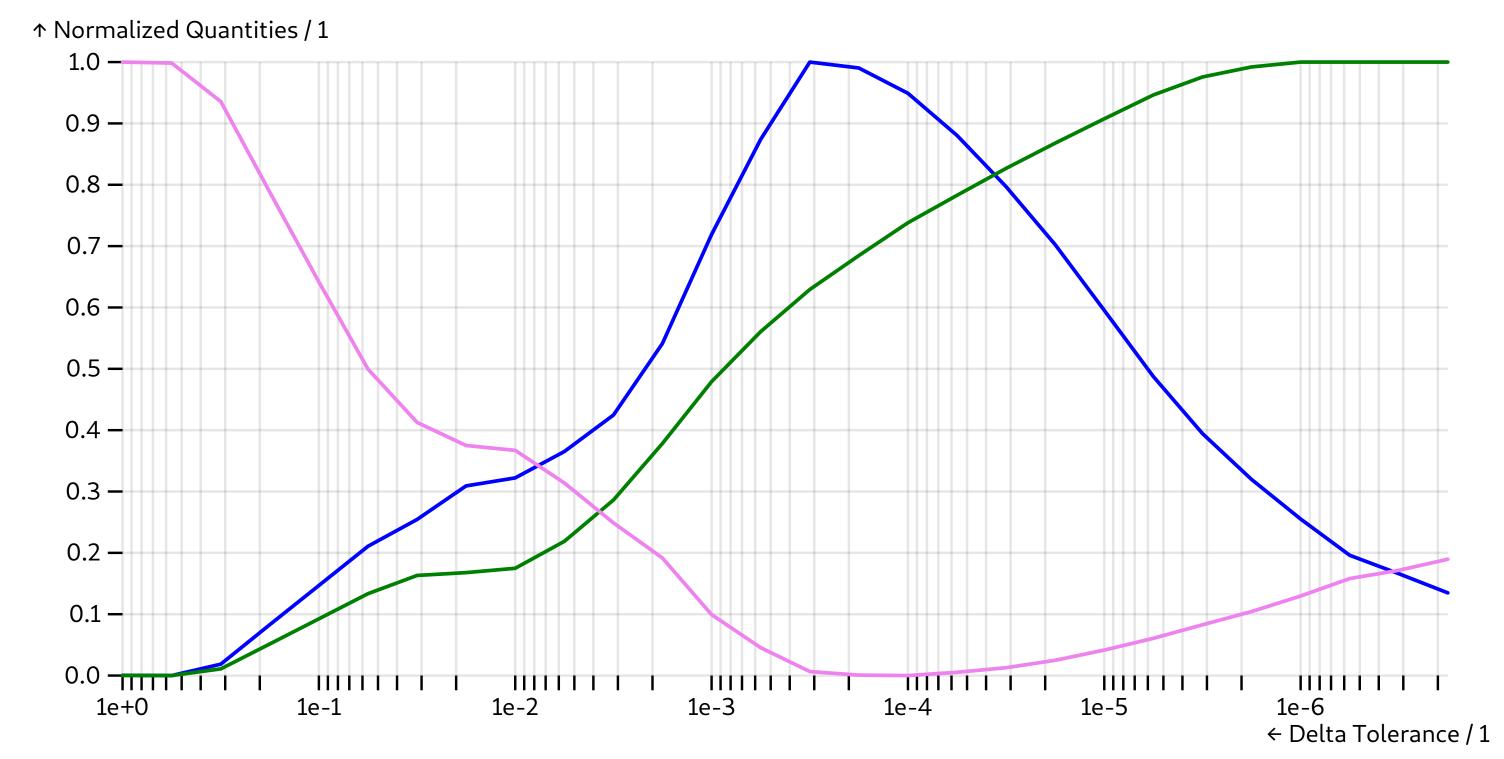
$$oldsymbol{s}_{k,n+1} = H_k\left(V(t_n), oldsymbol{C}(t_n), t_n
ight) oldsymbol{s}_{k,n} \,, \quad ext{with} \quad t_n := \sum\limits_{i=0}^n (\Delta t)_i \,.$$

ADAPTIVE TIMESTEPPING

In order to accelerate the simulation in areas where there is little change to the dynamics, we choose an adaptive step size $(\Delta t)_n$ based on

$$(\Delta t)_{n+1} = (\Delta t)_n \left(\frac{\Delta^{\mathrm{tol}}}{\sum_{k=1}^{M} N_k \|\boldsymbol{s}_{k,n+1} - \boldsymbol{s}_{k,n}\|_2} \right)^{1/2}.$$

In order to find the optimal $\Delta^{tol} \in \mathbb{R}^+$ (the allowed state change in between steps):



Relative change of the average timestep Δt (in blue), simulation runtime (in violet) and step acceptance rate (in green) when varying the delta tolerance $\Delta^{\rm tol}$ on a log-scale. All three quantities were normalized from their individual extent to [0,1]. The most effective $\Delta^{\rm tol}$ is arguably on the order of 10^{-4} .

FORMULATION AS A QUADRATIC PROGRAM

After simulation of the individual channel currents, we want to find

$$oldsymbol{N}_{ ext{opt}} = rg\min_{oldsymbol{N} \in \mathbb{N}_0^M} rac{1}{2} \left\| R oldsymbol{N} - oldsymbol{I}_{ ext{meas}}
ight\|_2^2 \ .$$

the number of channels per type, with $I_{\text{meas}} \in \mathbb{R}^{N_t}$ the experimentally measured current and $R \in \mathbb{R}^{N_t \times M}$ the matrix of all currents I_k per channel type. Letting $d := I_{\text{meas}}$ for brevity,

$$oldsymbol{N}_{ ext{opt}} pprox rg \min_{oldsymbol{x} \in \mathbb{R}^M} f(oldsymbol{x}) = rg \min_{oldsymbol{x} \in \mathbb{R}^M} rac{1}{2} \left\| Roldsymbol{x} - oldsymbol{d}
ight\|_2^2 \ ,$$

with cost function $f: \mathbb{R}^M \to \mathbb{R}^+$, which we manipulate to

$$f(\boldsymbol{x}) = \frac{1}{2}(R\boldsymbol{x} - \boldsymbol{d})^{T}(R\boldsymbol{x} - \boldsymbol{d})$$

$$= \frac{1}{2}(\boldsymbol{x}^{T}R^{T}R\boldsymbol{x} - \boldsymbol{x}^{T}R^{T}\boldsymbol{d} - \boldsymbol{d}^{T}R\boldsymbol{x} + \boldsymbol{d}^{T}\boldsymbol{d})$$

$$= \frac{1}{2}(\boldsymbol{x}^{T}P\boldsymbol{x} + \boldsymbol{x}^{T}\boldsymbol{q} + \boldsymbol{q}^{T}\boldsymbol{x}) + \mathcal{O}(1)$$

$$= \frac{1}{2}\boldsymbol{x}^{T}P\boldsymbol{x} + \boldsymbol{q}^{T}\boldsymbol{x} + \mathcal{O}(1)$$

where we let $P := R^T R \in \mathbb{R}^{M \times M}$ and $\mathbf{q} := -R^T \mathbf{d} \in \mathbb{R}^M$ and leave out the constant $\mathbf{d}^T \mathbf{d}$ as $\mathcal{O}(1)$. We can express the nonnegativity constraint $\mathbf{x} \geq \mathbf{0}$ as an equality constraint using a slack variable $\mathbf{s} \in \mathbb{R}^M_+$,

$$-\boldsymbol{x}+\boldsymbol{s}=\boldsymbol{0}$$
 \Leftrightarrow $A\boldsymbol{x}+\boldsymbol{s}=\boldsymbol{b}$ with $A=-\mathbb{1}\in\mathbb{R}^{M\times M}$ and $\boldsymbol{b}=\boldsymbol{0}\in\mathbb{R}^{M}$.

This leaves us with a constrained quadratic program,

$$\min_{oldsymbol{x} \in \mathbb{R}^M} \frac{1}{2} oldsymbol{x}^T P oldsymbol{x} + oldsymbol{q}^T oldsymbol{x}, \ s.t. \ A oldsymbol{x} + oldsymbol{s} = oldsymbol{b} \ , \ oldsymbol{s} \in \mathbb{R}_+^M \ .$$

The integer solution can then be obtained from rounding,

$$oldsymbol{N}_{ ext{opt}} = \lfloor oldsymbol{x}
ceil \in \mathbb{N}_0^M$$
 .

COMPARISON OF OPTIMIZATION METHODS

The different approaches were evaluated on the G0 cell cycle phase with the activation voltage protocol. Runtime estimates were obtained on an IntelTMi7-5600U CPU.

Algorithm	Abbreviation	Runtime / ms	RMSE / pA
Particle Swarm Optimization	PSO	22571	27.69
Gradient Descent + More Thuente	GD	18924	32.34
Limited-Memory BFGS + Hager Zhang	LBFGS	4845	32.20
Non-Negative Least Squares [3]	NNLS	318	28.00
Quadratic Program	QP	18	28.13

CONCLUSION

Efforts to further enhance and complete the first electrophysiological cancer cell model simulation were fruitful, resulting in a new library implementation, an improved inverse problem solution technique and a live in-browser simulation dashboard. Numerically, the stability of the simulation varies greatly with the time step state change tolerance Δ^{tol} , this could be improved using a higher-order integration scheme. There are also many ideas for further customizations that would improve the live simulation dashboard, opening up future usage perspectives.

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