

# Synthetic Segmented Virtual Head Model Generation Using Generative Adversarial Network (GAN)

**NAHIAN IBN HASAN**

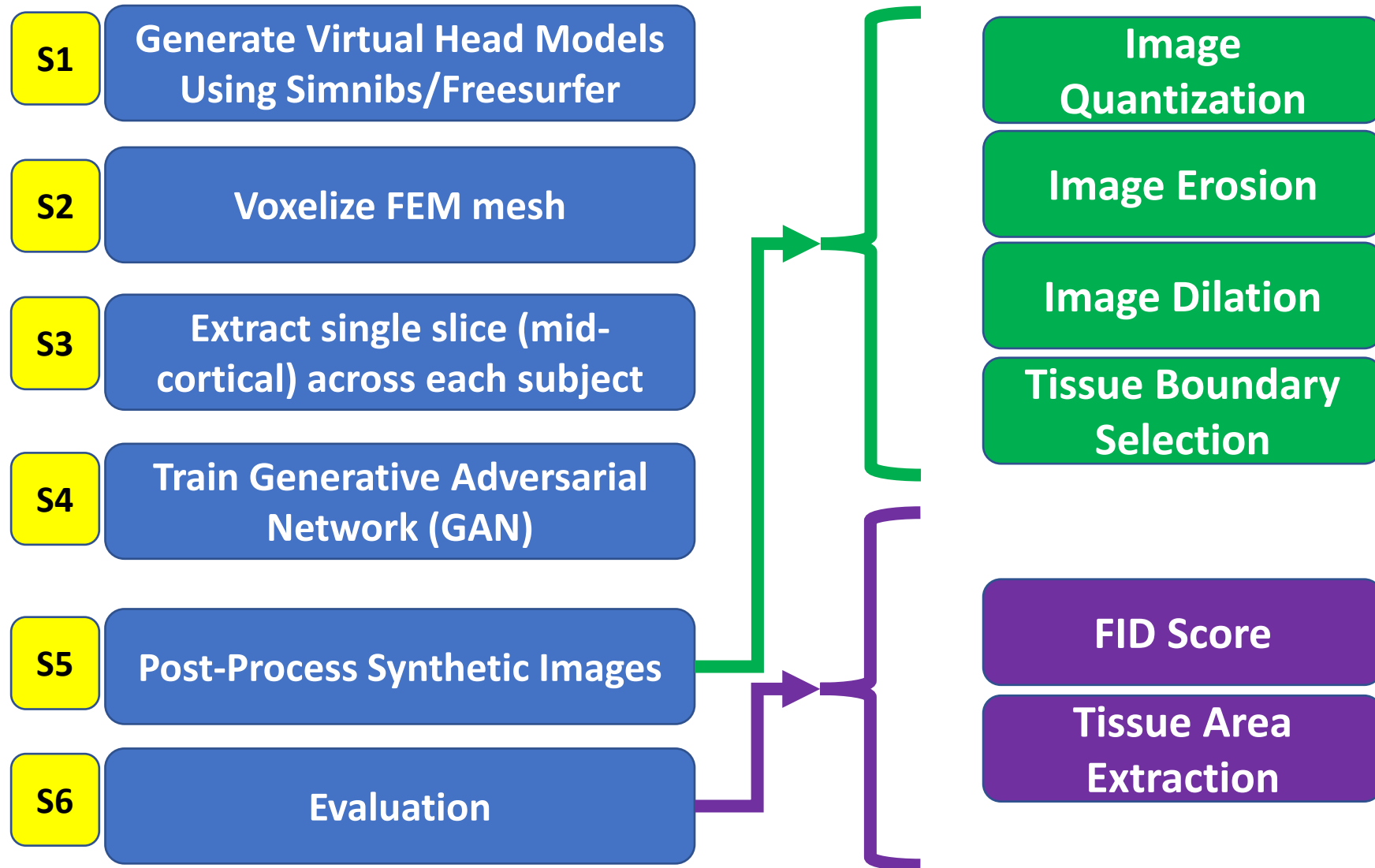
Elmore School of Electrical and Computer Engineering  
Purdue University, West Lafayette (WL), IN, USA



## **The Purpose of Generating Synthetic Data**

- .Data Augmentation for MRI images for Machine Learning Projects**
- .Population based studies and uncertainty quantification**
- .Image Super-resolution (1.5T MRI → 3T/5T/7T MRI)**

# Project Workflow



**Database** : Wu-Minn Human Connectome Project [1]

- Data Type : Structural MRI scans
- Coil Type : 3T/7T
- MRI type : T1w and T2w
- Number of Subjects : 812
- Subject Age : 22-35
- Ratio M/F : (47/53) %

[1] <https://www.humanconnectome.org/study/hcp-young-adult/document/1200-subjects-data-release>

# Step 1 – Real Virtual Head Model Generation



MRI Scans

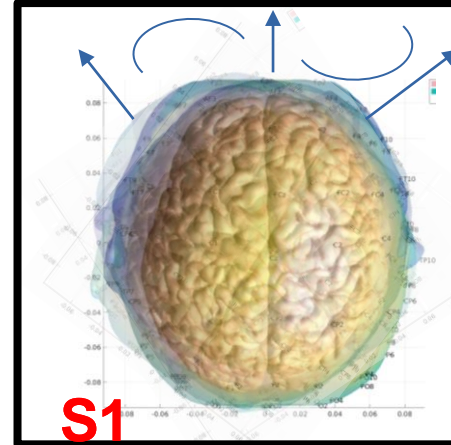
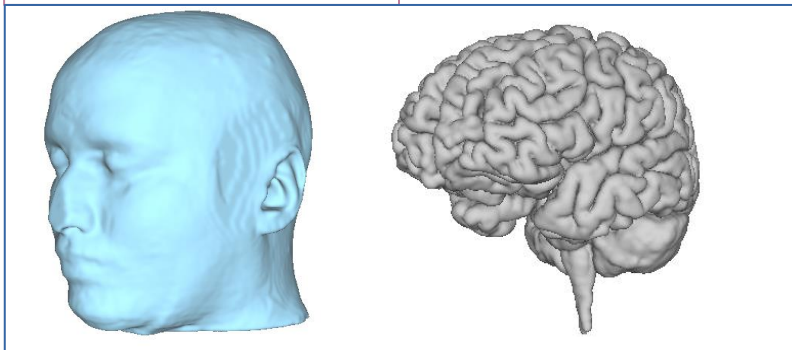
## SimNIBS Uses Freesurfer\* for Surface Based Cortical Tissue Segmentation

- S1. Co-registration
- S2. B-field in-homogeneity correction
- S3. Skull-stripping
- S4. Segment based on GM/WM
- S5. Divide Brain into LH and RH

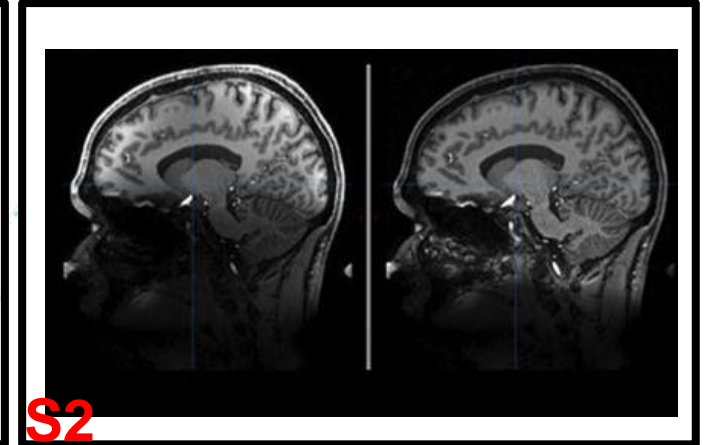
## For each Hemisphere:

- S6. Fill holes of the WM
- S7. Deform triangle mesh to fit GM/WM interfaces

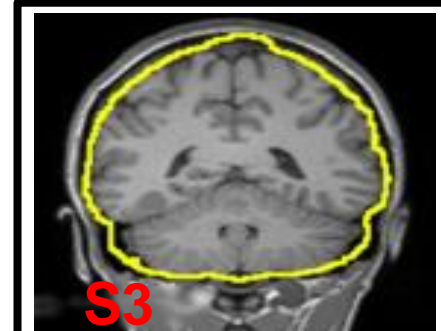
Virtual Head Model



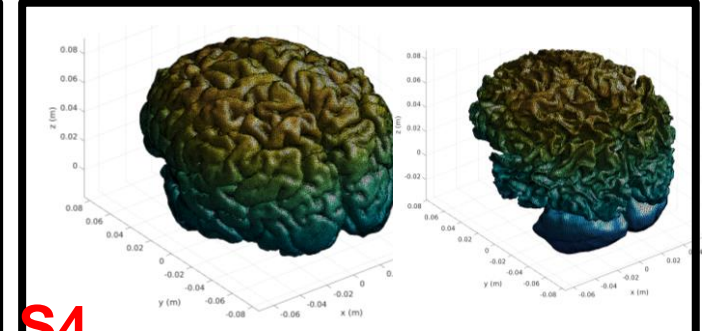
S1



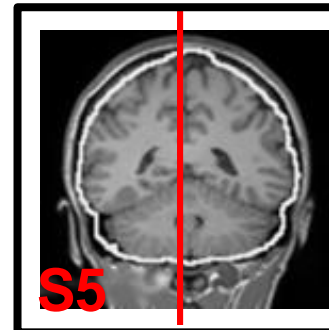
S2



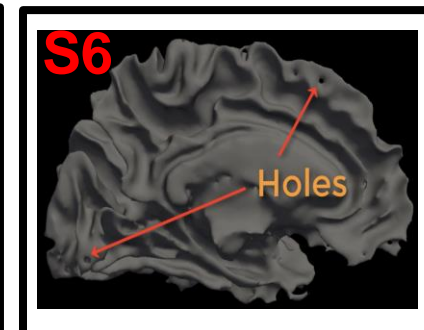
S3



S4



S5



S6

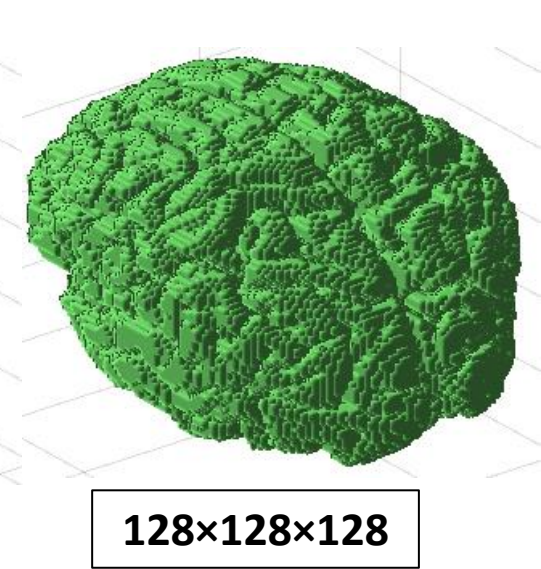
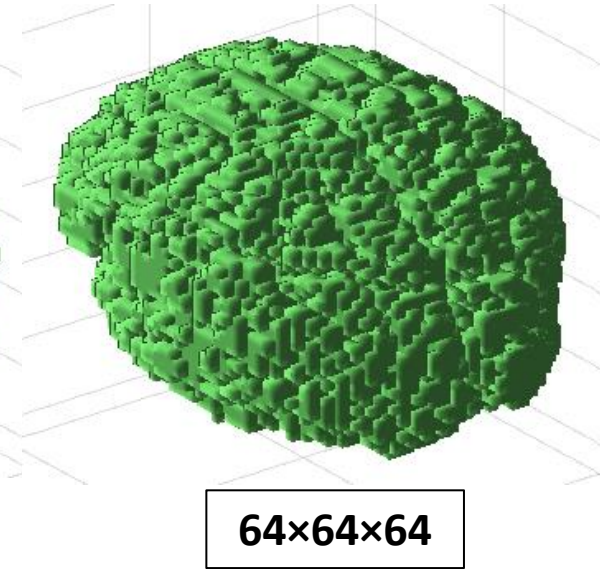
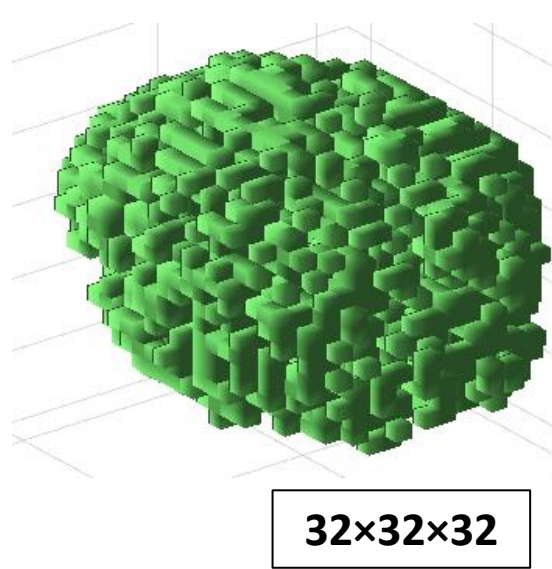
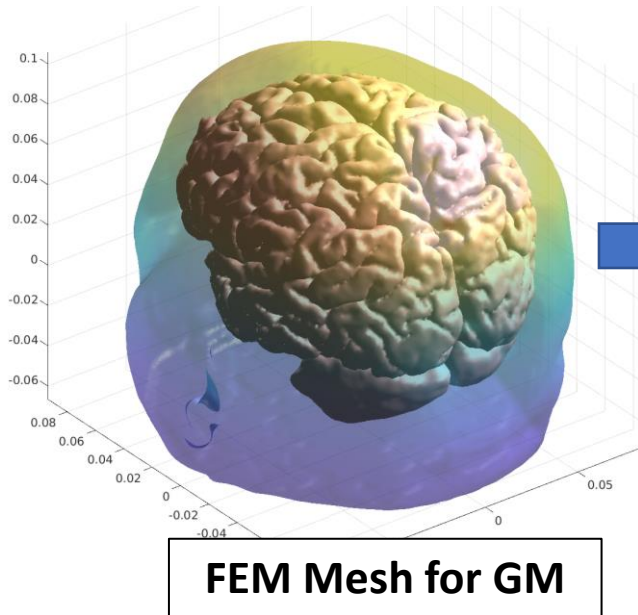
Holes



S7

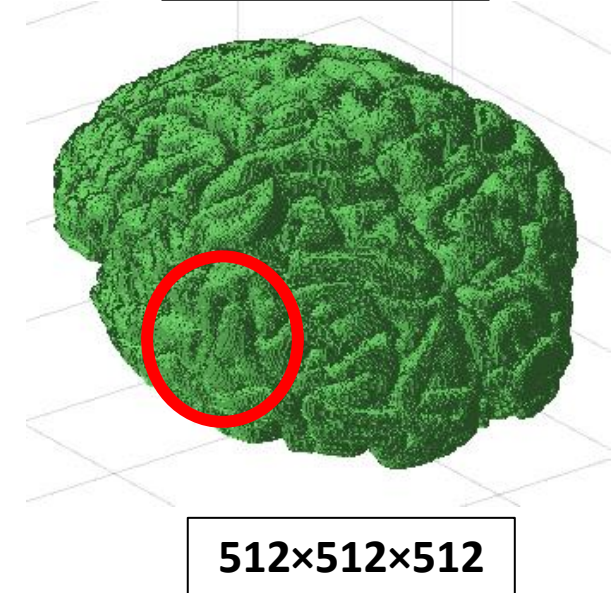
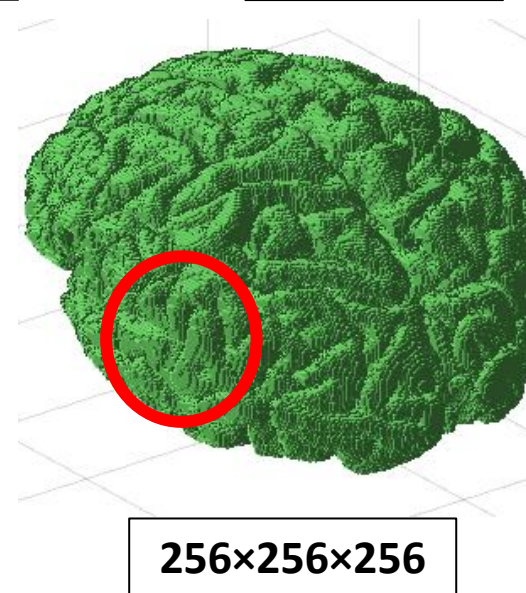


# Step 2 – Voxelization of FEM Mesh

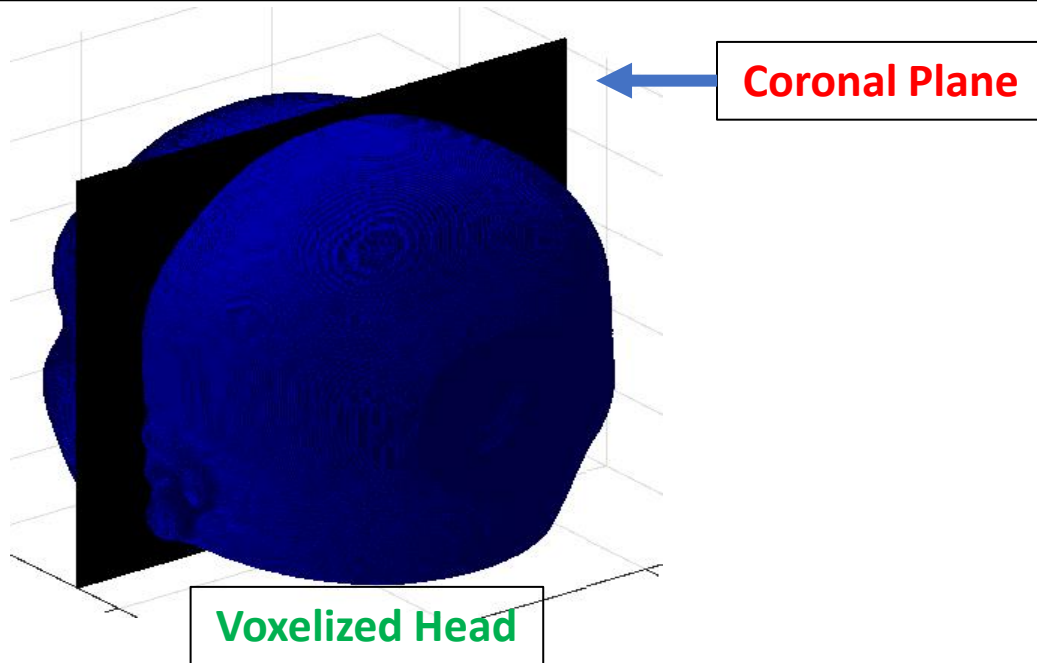


## Effect of Voxelization Grid

- For lower grid dimensions-
  1. Uncertainty in tissue boundary
  2. Greater staircase effect
- For higher grid dimensions-
  1. Computational Effect (Higher Memory)

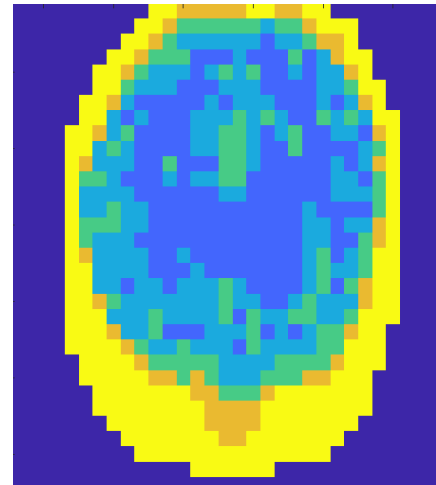


# Step 3 – Extract Mid-Cortical Slice (Coronal Plane)

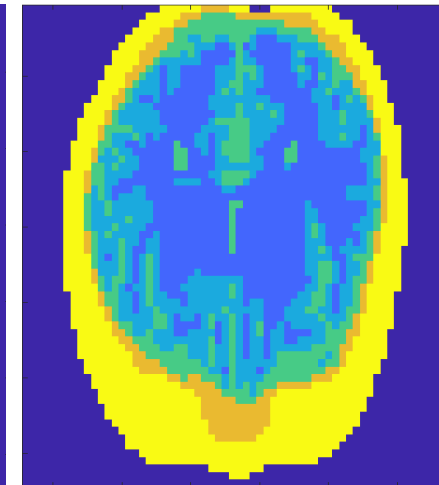


## Effect of Voxelization Grid

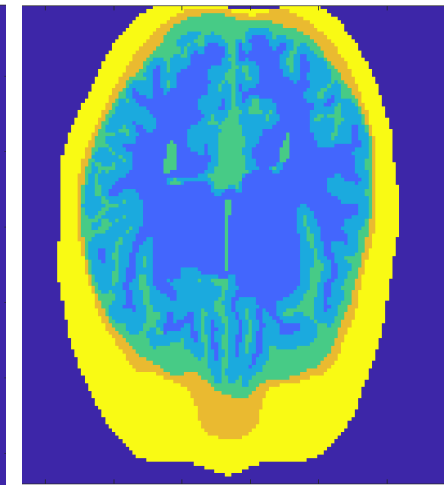
- For lower grid dimensions-
  1. Uncertainty in tissue boundary
  2. Greater staircase effect
- For higher grid dimensions-
  1. Computational Effect (Higher Memory)



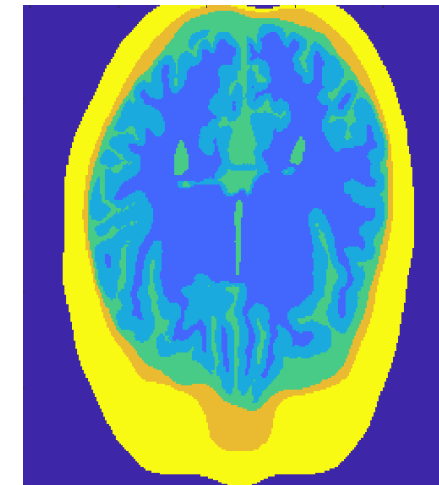
32×32



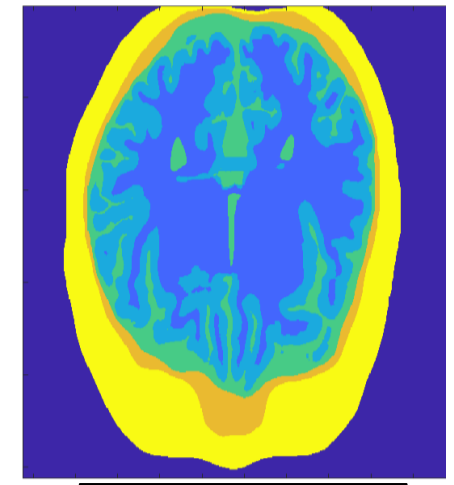
64×64



128×128

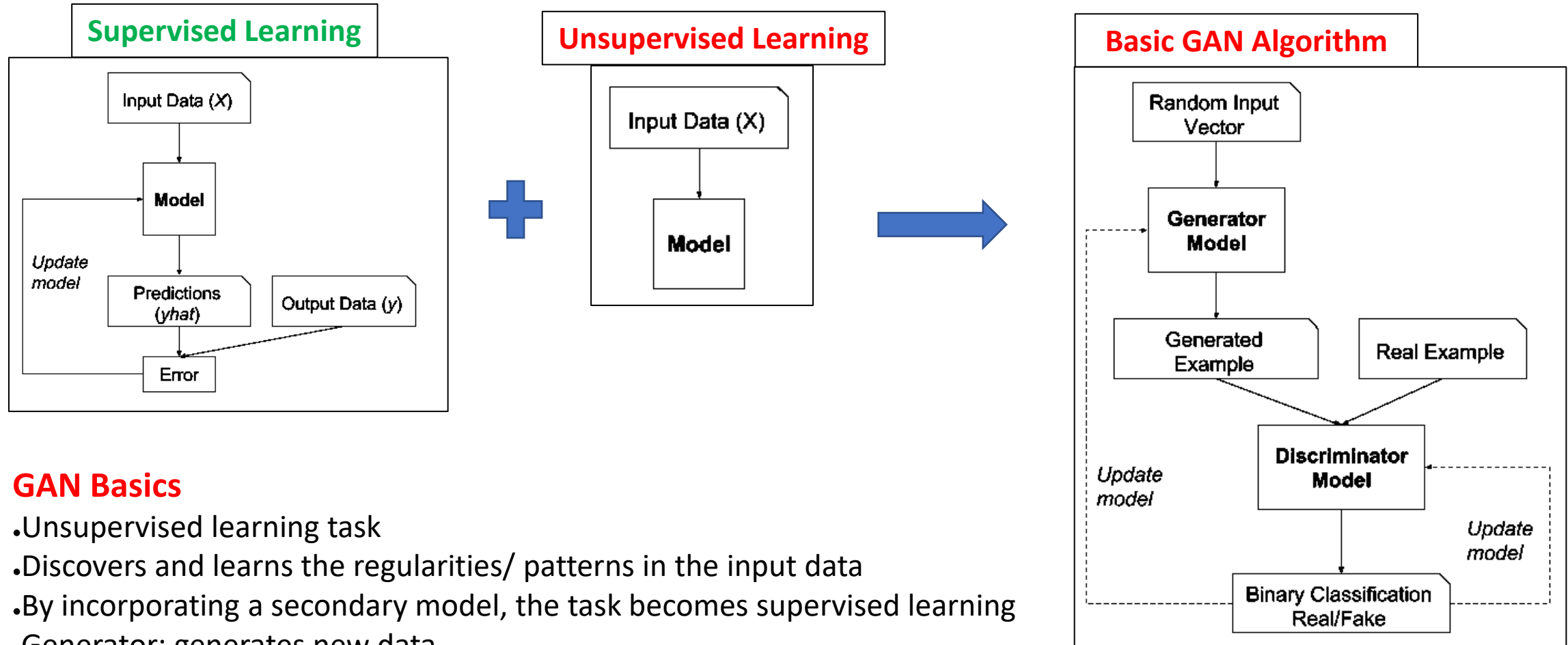


256×256



512×512

# Generative Adversarial Network (GAN)



## GAN Basics

- Unsupervised learning task
- Discovers and learns the regularities/ patterns in the input data
- By incorporating a secondary model, the task becomes supervised learning
- Generator: generates new data
- Discriminator: discriminates between real and generated/fake image



# Generative Adversarial Network (GAN)-Examples



2014

2015



2016

2017



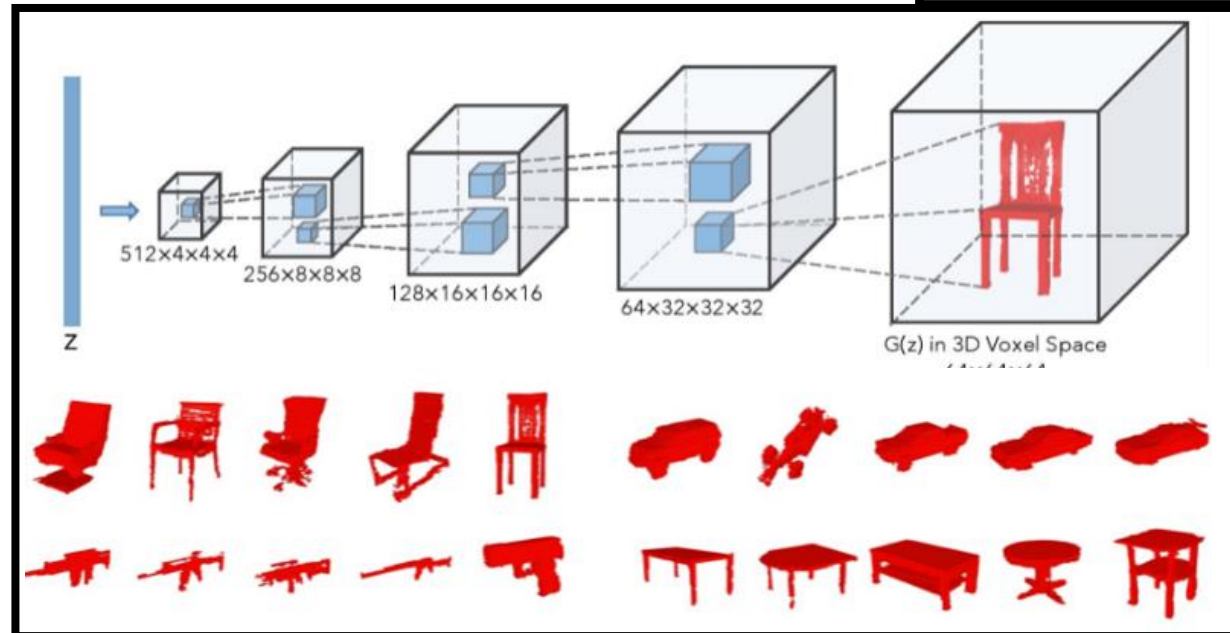
2019

2020

## Types of GAN

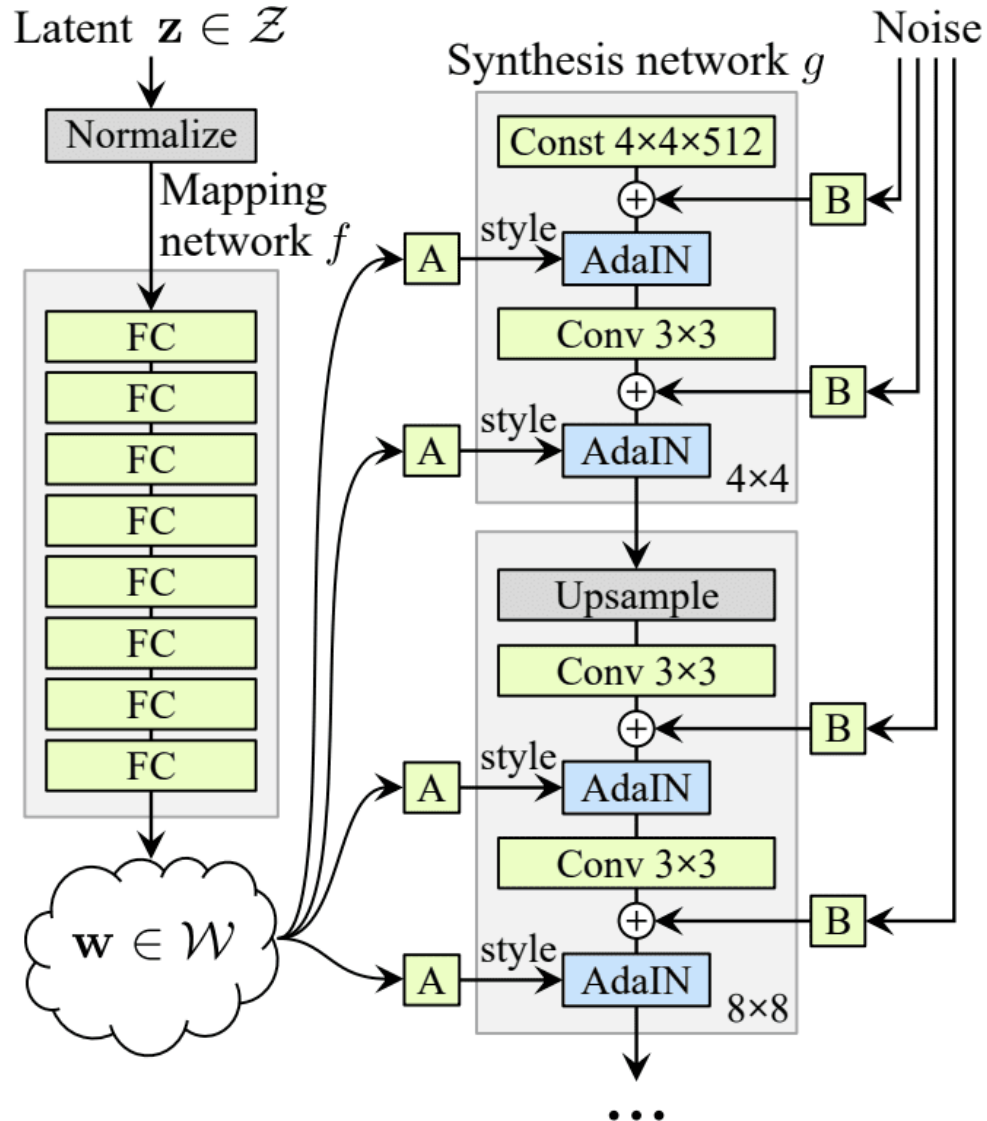
- DCGAN----- deep convolutional GAN
- Conditional GAN----conditional data generation
- BigGAN
- StyleGAN
- Pix-to-Pix----- Image Translation
- CycleGAN-----Image Translation
- Progressive Growing GAN

## 3D GAN[\*]



[\*]Wu, J., Wang, Y., Xue, T., Sun, X., Freeman, W. T., & Tenenbaum, J. B. (2017). Marnet: 3d shape reconstruction via 2.5 d sketches. *arXiv preprint arXiv:1711.03129*.

# Step 4 – Training Generative Adversarial Network (StyleGAN)



## StyleGAN[\*] Basics

- Baseline Progressive GAN.
- Addition of tuning and bilinear upsampling.
- Addition of mapping network and AdaIN (styles).
- Removal of latent vector input to generator.
- Addition of noise to each block.
- Addition Mixing regularization.

$$\text{AdaIN}(x_i, y) = y_{s,i} \frac{x_i - \mu(x_i)}{\sigma(x_i)} + y_{b,i}$$



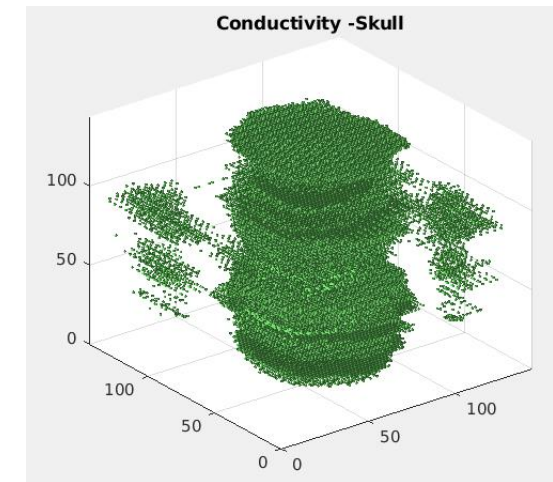
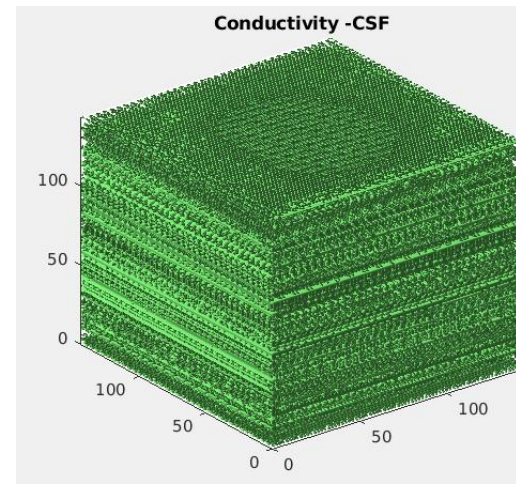
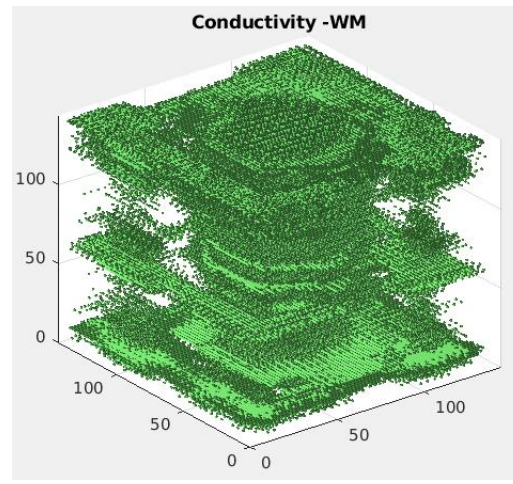
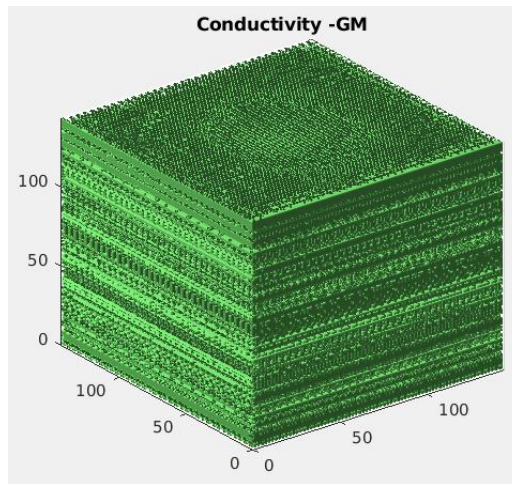


# Step 4 – Training Generative Adversarial Network (StyleGAN)

## Attempt 1 (3D GAN – All Tissues)

- DCGAN – 3D convolution on 3D data
- Generator Network - Unet, AlexNet, Resnet50, ResNet152, Xception

## Resultant Images: random 3D data

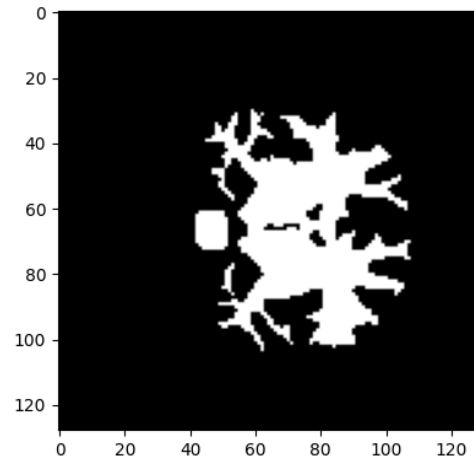


# Step 4 – Training Generative Adversarial Network (StyleGAN)

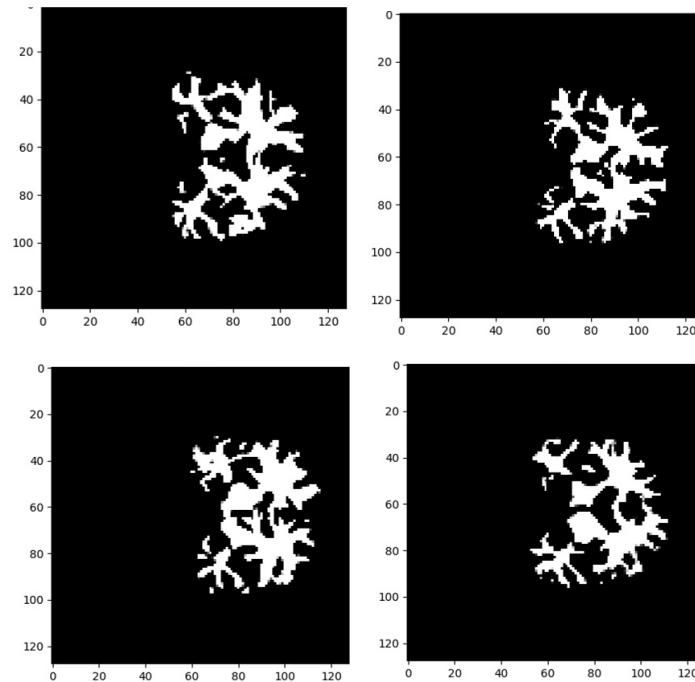
## Attempt 2 (2D GAN – Single Tissue)

•StyleGAN – 2D convolution for single slice and single tissue (WM)

### Resultant Images



Original WM



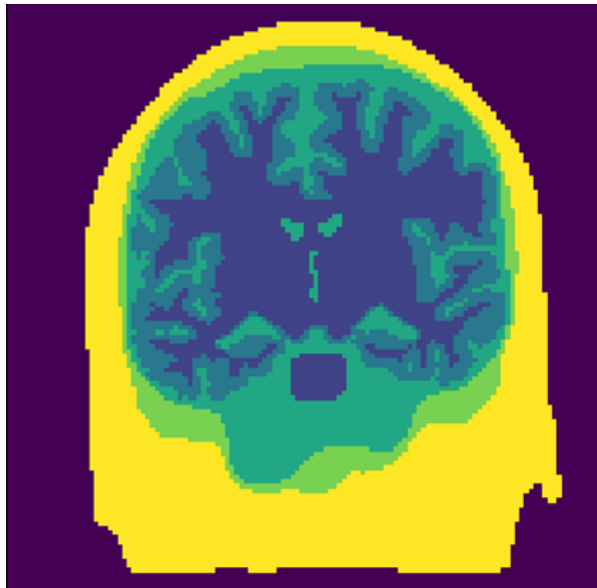
Synthetic WM

# Step 4 – Training Generative Adversarial Network (StyleGAN)

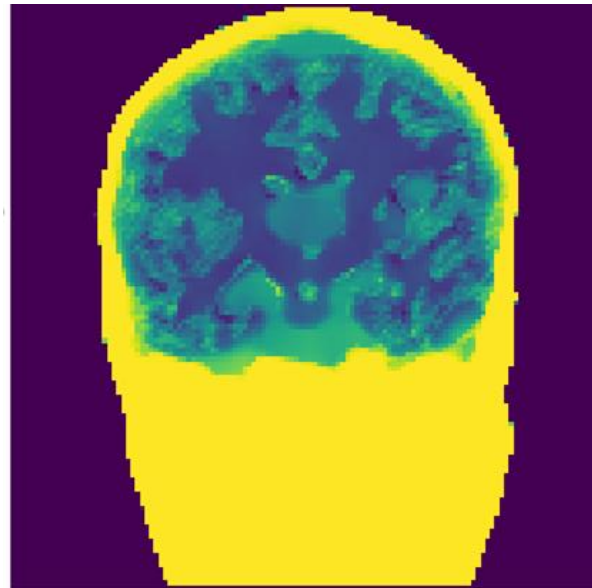
## Attempt 3 (2D GAN – All Tissues)

•StyleGAN – 2D convolution for all tissues (WM, GM, CSF, Skull, Scalp)

### Resultant Images



Original MRI Slice

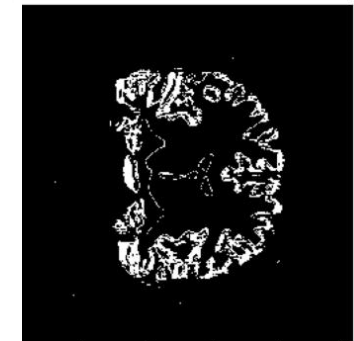


Synthetic MRI Slice

WM



GM



Scalp

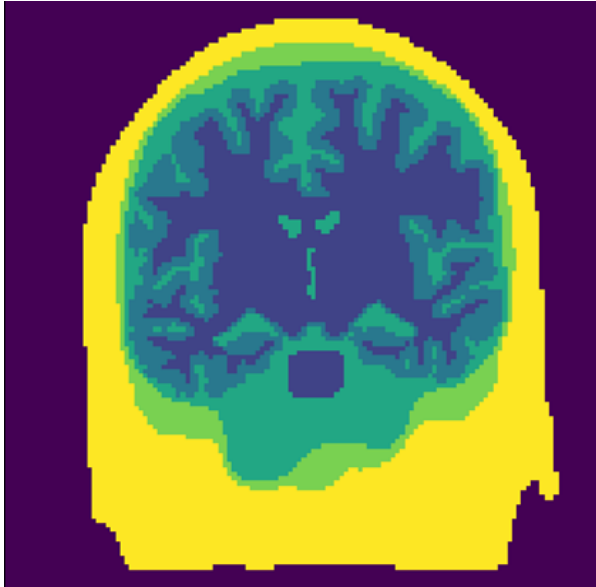


Extracted  
From  
Synthetic  
Slice

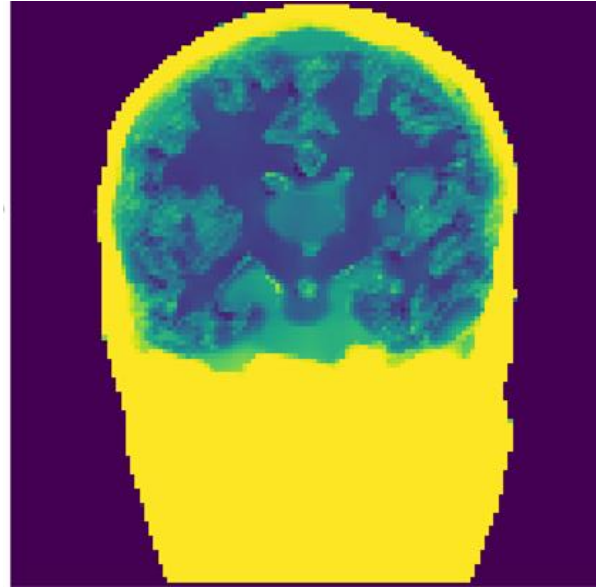


# Step 5 – Post-Process Synthetic Slices

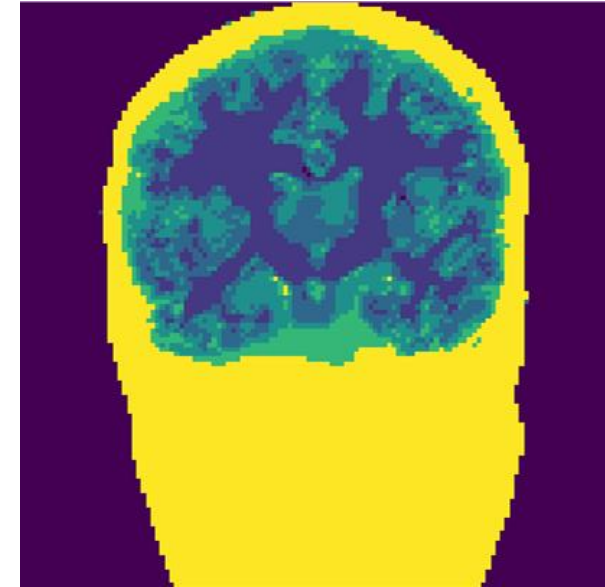
## Step 5.1 – Image Quantization



Original MRI Slice



Synthetic MRI  
Slice



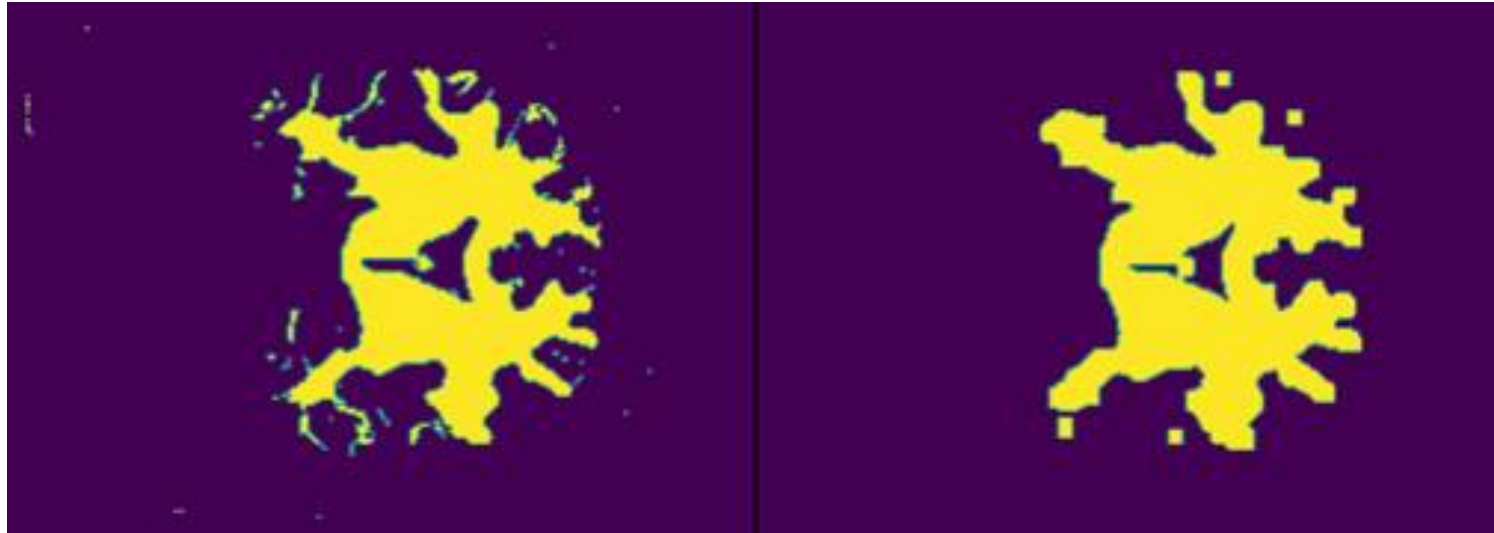
Quantized MRI  
Slice

### Purpose of Image Quantization

- GAN generated images are floating point samples from inherent latent space
- Quantization labels each pixel of certain tissue type [1-6]
- We implemented quantization by thresholding on histogram on generated image

# Step 5 – Post-Process Synthetic Slices

## Step 5.2 – Image Erosion and Dilation

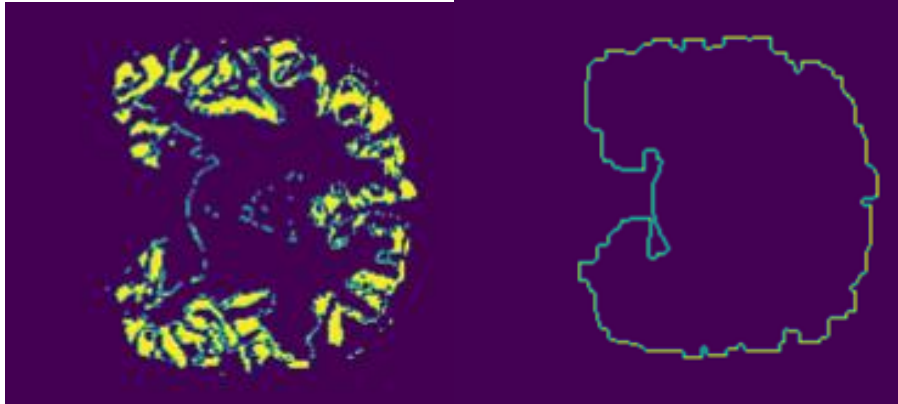


### Purpose of Image Erosion and Dilation

- Image Erosion removes small noises
- Image Dilation fills the missing data points in a continuous contour.
- Erosion + Dilation = **Image Opening**
- Dilation + Erosion = **Image Closing**

# Step 5 – Post-Process

## Step 5.3 – Contour Selection



Outer Boundary - GM

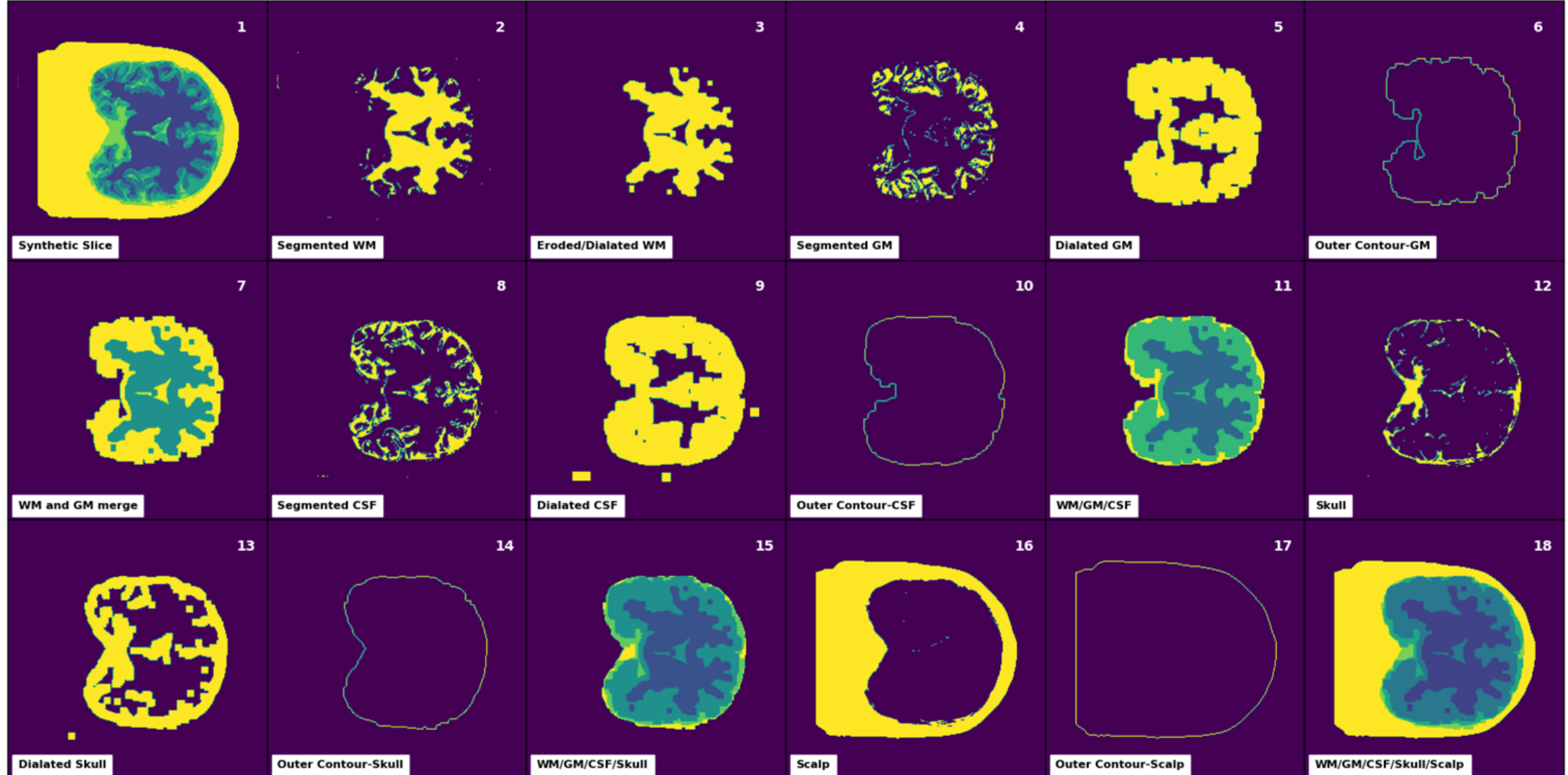


Outer Boundary - CSF

### Purpose of Image Contour Selection

- To find the tissue boundary

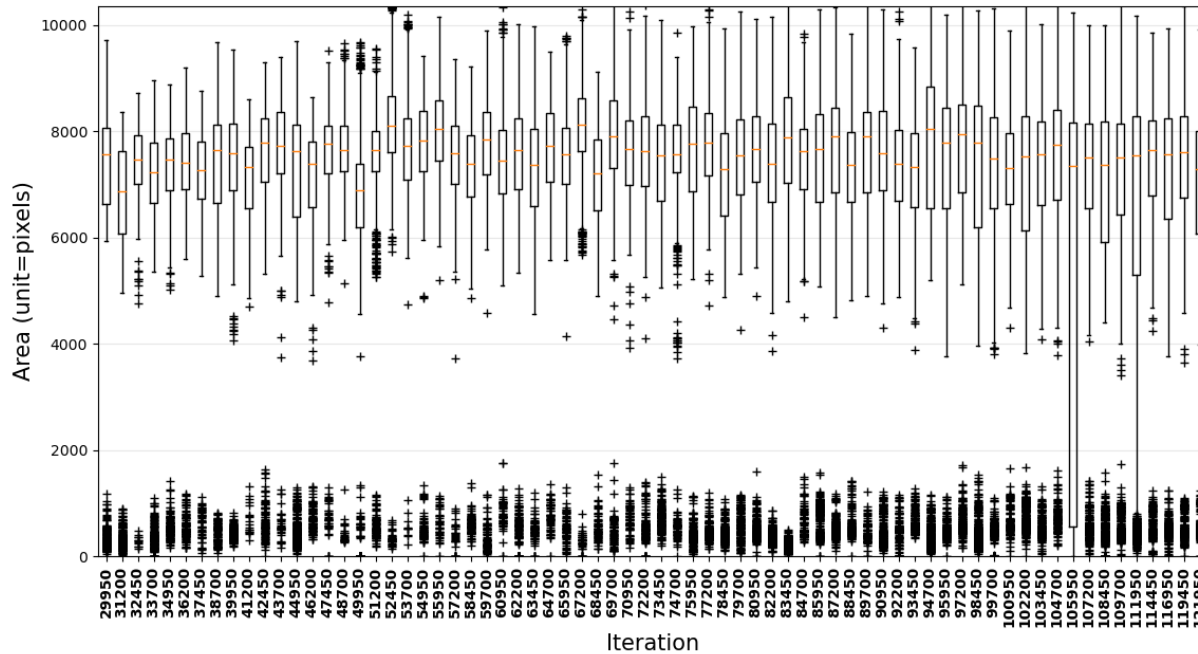
# Step 5 – Summary of Post-Processing



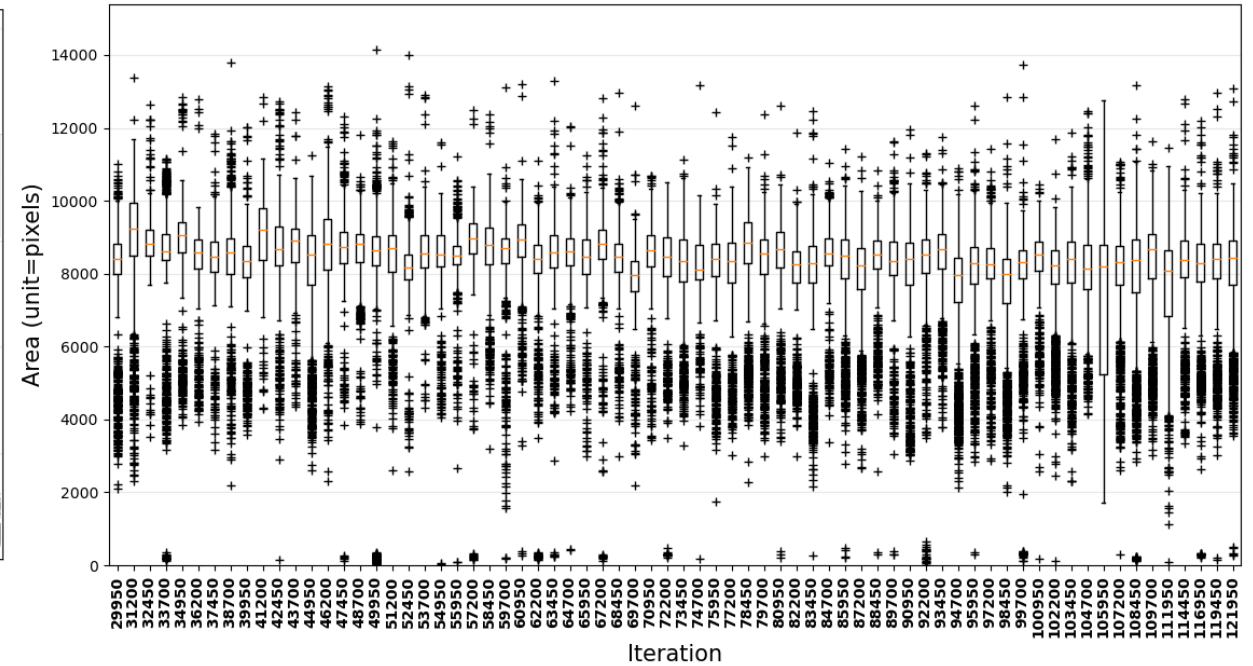
# Step 6 – Evaluation of GAN-Generated Synthetic Images

## Step 6.1 : Tissue Area

.Tissue Area = Number of Pixels × Pixel Area



White Matter



Gray Matter

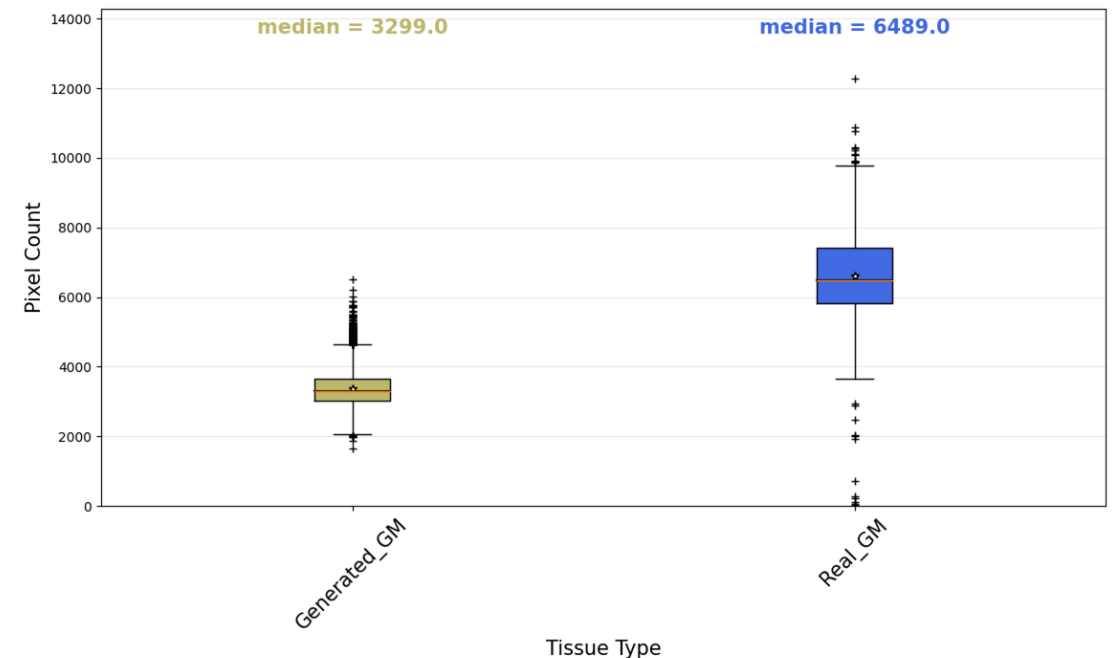
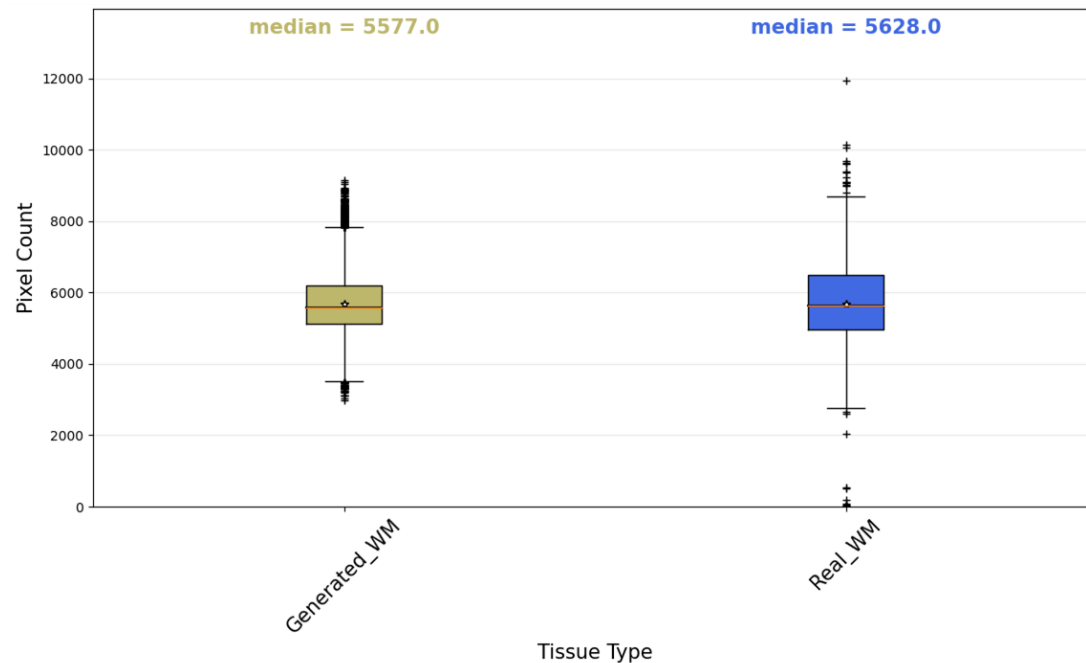
**Summary:** Tissue Area doesn't provide any insight about the quality of generated image



# Step 6 – Evaluation of GAN-Generated Synthetic Images

## Step 6.2 : Tissue Area Comparison

• Tissue Area = Number of Pixels × Pixel Area

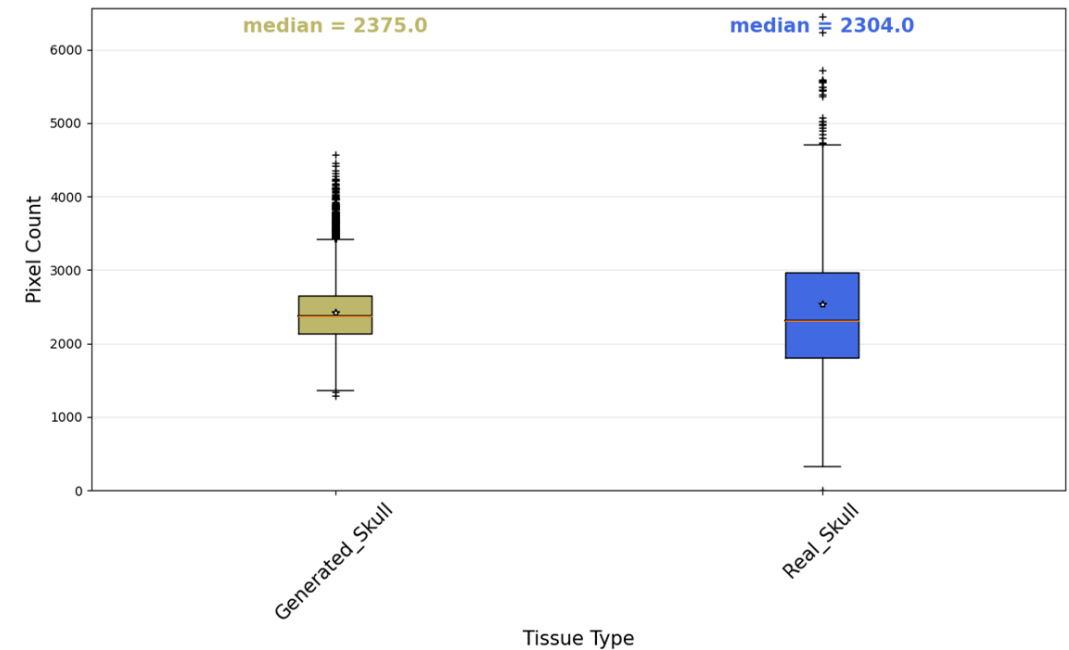
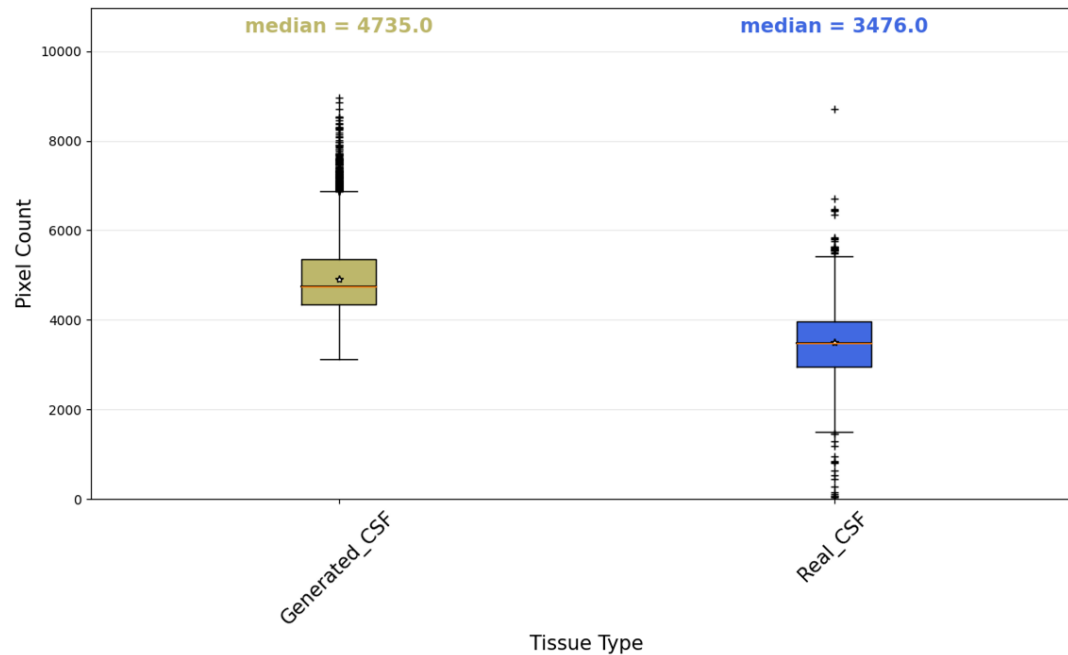


**Summary:** Tissue area of synthetic images resembles the tissue area of ground truth data

# Step 6 – Evaluation of GAN-Generated Synthetic Images

## Step 6.2 : Tissue Area Comparison

• Tissue Area = Number of Pixels × Pixel Area



**Summary:** Tissue area of synthetic images resembles the tissue area of ground truth data

# Step 6 – Evaluation of GAN-Generated Synthetic Images

## Step 6.3 : Frechet Inception Distance (FID Score)

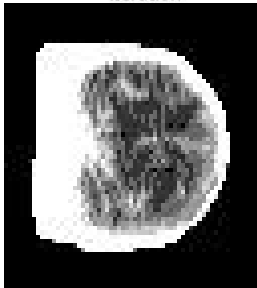
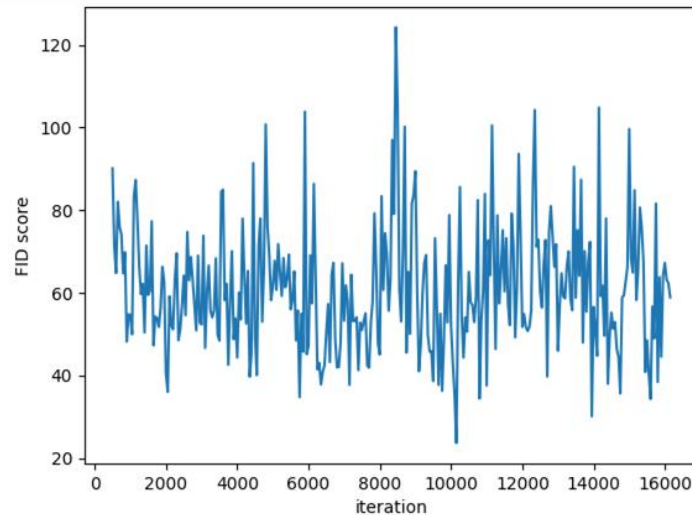
$$d^2 = ||\mu_1 - \mu_2||^2 + \text{Tr}(C_1 + C_2 - 2 \times \sqrt{C_1 \times C_2})$$

- $\mu_1, \mu_2$  = mean of the probability vectors at the output of Inception V3 network
- $C_1, C_2$  = covariance matrices
- $\text{Tr}$  = Trace of the matrix
- **We want the FID score to be as low as possible**

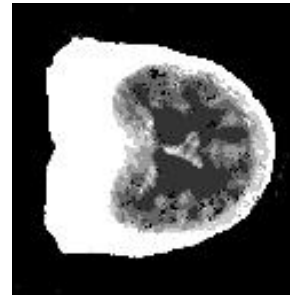
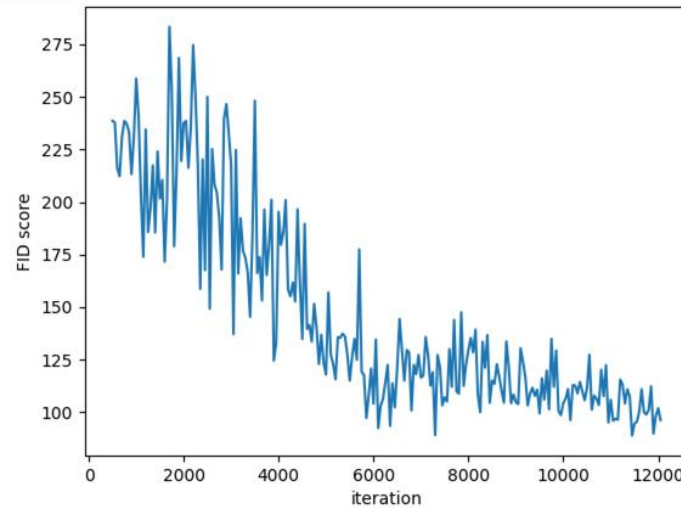
# Step 6 – Evaluation of GAN-Generated Synthetic Images

## Step 6.3 : Frechet Inception Distance (FID Score)

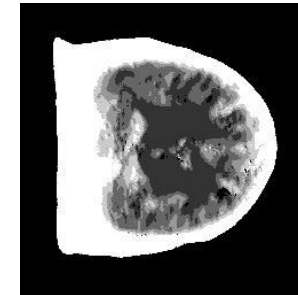
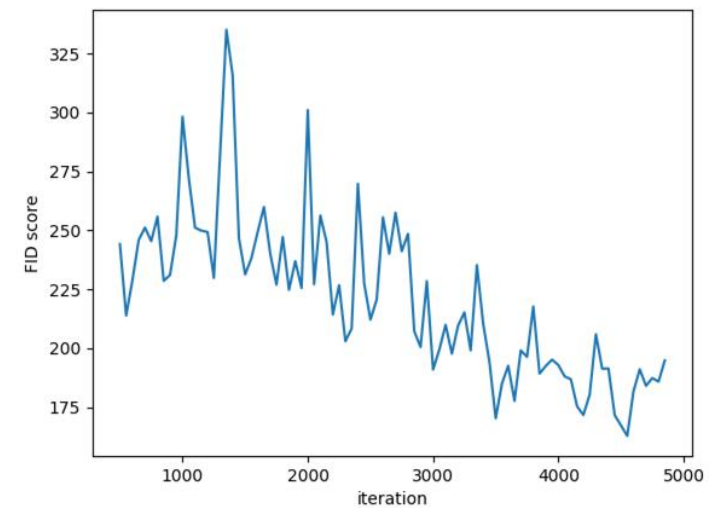
• Each iteration – 5000 generated samples



64×64



128×128



256×256

# Summary of Project Outcome

1. The voxelization grid size affects the image quality, especially tissue boundary.
2. StyleGAN generated synthetic images require a substantial number of iterations before generating any meaningful image that resembles a ground truth MRI image.
3. The area of any tissue does not predict the quality of synthetic image at any training iteration.
4. The inception score does not provide a good estimation of the synthetic image.
5. The FID score improves with respect to training iterations. But it is meaningful for higher voxelization grid size.
- 6. The FID score can be used as a parameter for statistical inference.**
7. Decision: Based on the current analysis the following configuration should be used for synthetic 2D MRI data generation—
  1. Network = StyleGAN
  2. Voxelization Grid Size =  $256 \times 256 \times 256$
  3. Evaluation Metric = FID score and manual inspection

## Drawback

1. The sliced images across subjects does not provide the same cortical plane across subject



## **Future Direction**

1. Use MNI coordinate system to extract the same cortical plane across subjects
2. Extend the concept to generate 3D virtual synthetic head model
3. Implement the 3D StyleGAN
4. Explore Multi-GPU processing technique to accommodate 3D volumetric data

# References

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**Thank You**

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