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DOI: 10.1038/s41467-024-44824-z
Review article
Nature Communications (2024)
Online: 22 January 2024

Context: Segmentation fondation models

• **SAM = segment anything model**, remarkable versatility and performance across various segmentation tasks

Advantages:

- Wide range of segmentation tasks for one training
- Could lead to more consistent results across different tasks

But in medical imaging...

Challenges:

• Significant differences between image modalities (3D/2D), imaging protocols and machines, etc.

- Segmentation task can vary depending on the specific clinical scenario
 (Example: segmenting the liver tumor VS entire liver and surroundings organs on CT scan)
 - Need of user provided prompts

MedSAM training and validation method

Fine-tuning SAM with:

- 1,570,263 image-mask pairs (unprecedented dataset; 80% training, 10% tuning, and 10% validation)
 - MRI/CT slices in **NifTI format** + [0, 255] intensity normalization + [1024×1024×3] resizing
 - Grayscale/RGB in png format + [1024×1024×3] resizing
- **10 images modalities**, with a multitude of imaging protocols
- 30 cancer types
- 86 internal validation tasks
- 60 external validation tasks
 - Unseen segmentation targets
 - New domains (cell segmentation in LM images and organelle segmentation in EM images)

Comparison with:

- SOTA segmentation foundation model SAM
- 10 dedicated specialist models based on U-Net and DeepLabV3+ respectively

MedSAM datasets distribution and MedSAM architecure

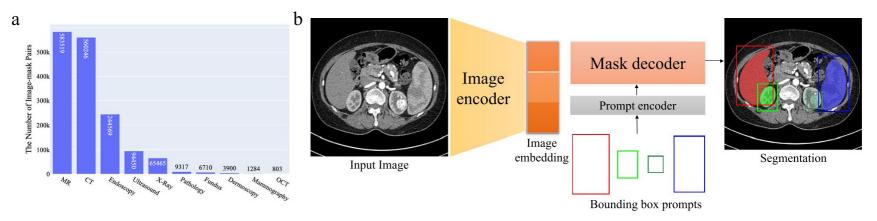
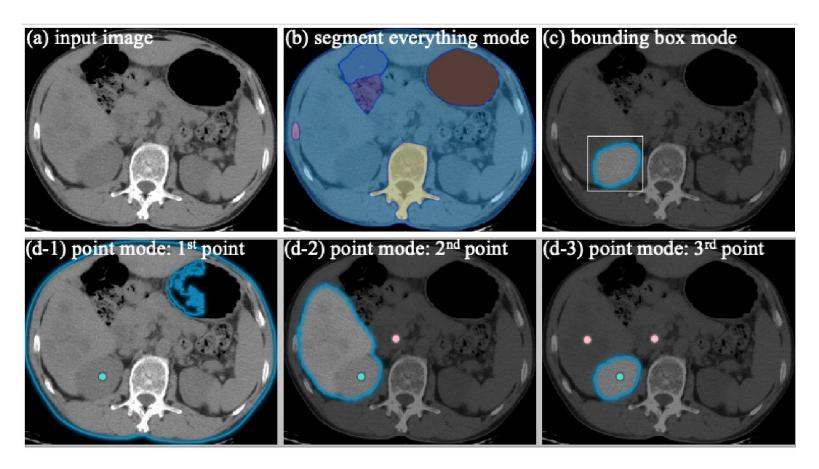


Fig. 2 | **Overview of the modality distribution in the dataset and the network architecture.** a The number of medical image-mask pairs in each modality. **b** MedSAM is a promptable segmentation method where users can use bounding boxes to specify the segmentation targets. Source data are provided as a Source Data file.

Modality	Num. of Training Images		
Computed Tomography	362,229		
Magnetic Resonance Imaging	442,818		
X-Ray	36915		
Mammography	986		
Optical Coherence Tomography	642		
Ultrasound	74761		
Dermoscopy	2955		
Endoscopy	194805		
Fundus	960		
Pathology	6239		

- Image encoder based on vision transformer:
 - 12 transformer layers
 - multi-head self-attention and multilayer perceptron per block
- Mask decoder:
 - feature size in image embedding of 64×64

MedSAM prompt types



MedSAM Loss function

Binary cross entropy loss:
$$L_{\text{BCE}} = -\frac{1}{N} \sum_{i=1}^{N} \left[g_i \log s_i + (1 - g_i) \log(1 - s_i) \right]$$

Dice loss:
$$L_{\text{Dice}} = 1 - \frac{2 \sum_{i=1}^{N} g_i s_i}{\sum_{i=1}^{N} (g_i)^2 + \sum_{i=1}^{N} (s_i)^2}$$

Total loss:
$$L = L_{BCE} + L_{Dice}$$

si, gi denotes the predicted segmentation and ground truth of voxel i, respectively.

N is the number of voxels in the image I.

MR image datasets

TABLE 2

Magnetic Resonance (MR) image datasets. Datasets marked with * denote external validation sets and the remaining datasets are used for internal validation.

internal validation.					
Dataset Name	Modality	Segmentation Targets	# of scar	ns	
ACDC* [30]	MR	Heart anatomies	150	https://humanheart-project.creatis.insa-lyon.fr/	
AMOS-MR [6]	MR	Abdominal organ	40	https://amos22.grand-challenge.org/Dataset/	
ATLAS R2.0 [31]	MR-T1	Brain stroke	1271	https://atlas.grand-challenge.org/	
Brain Tumor Dataset Figshare [32], [33]	MR-T1ce	Brain tumor	233	https://www.kaggle.com/datasets/ashkhagan/	
Brain TR-GammakKnife [34]	MR	Brain lesion	47	https://doi.org/10.7937/xb6d-py67	
BraTS [35]-[39]	MR-T1, MR-T1CE, MR-T2, MR-FLAIR	Brain tumor		http://braintumorsegmentation.org/	
CC-Tumor Heterogeneity* [40]	MR	Cervical cancer		https://doi.org/10.7937/ERZ5-QZ59	
CHAOS* [41]	MR-T1, MR-T2	Liver, kidney, spleen	60	https://chaos.grand-challenge.org/	
crossMoDA [42]	MR	Brain tumor		https://crossmoda-challenge.ml/	
FeTA [42]	MR-Fetal	Brain tissues		https://feta.grand-challenge.org/	
HaN-Seg* [43]	MR	Head organs		https://zenodo.org/record/	
ISLES 44	MR-DWI, MR-ADC, MR-FLAIR	Ischemic stroke lesion		http://www.isles-challenge.org/	
I2CVB [45]	MR-T2, MR-DWI	Prostate		https://i2cvb.github.io/	
Meningioma-SEG-CLASS [46]	MR-T1ce, T2-FLAIR	Tumor (meningioma)		https://doi.org/10.7937/0TKV-1A36	
MMs [47]	MR	Heart anatomies		https://www.ub.edu/mnms-2/	
MSD-Heart [48]	MR	Left atrial		http://medicaldecathlon.com/	
MSD-Prostate [21]	MR-ADC, MR-T2	Prostate		http://medicaldecathlon.com/#tasks	
NCI-ISBI [49]	MR-ADC, MR-T2	Prostate		http://dx.doi.org/10.7937/K9/TCIA.2015.zF0vl	
PI-CAI 50	MR-bp	Prostate cancer		http://github.com/DIAGNijmegen/picai_labels	
PPMI [51]	MR-T1	Brain regions of Parkinson patients		https://www.ppmi-info.org/access-data-specin	
PROMISÉ [52]	MR-T2	Prostate		https://promise12.grand-challenge.org/Details/	
Qin-Prostate-Repeatability [21], [53]	MR	Left atrium		http://doi.org/10.7937/K9/TCIA.2018.MR1CK0	
QUBIQ* [54]	MR	Prostate		https://qubiq21.grand-challenge.org/	
Spine [55]	MR	Vertebrae		https://www.cg.informatik.uni-siegen.de/en/sp	
ŴMH [56]	MR-T1, MR-FLAIR	White matter hyper-intensities	60	https://wmh.isi.uu.nl/	

Evaluation metrics

$$\mathrm{DSC}(G,\,S) \,=\, rac{2|G\cap S|}{|G|+|S|}$$

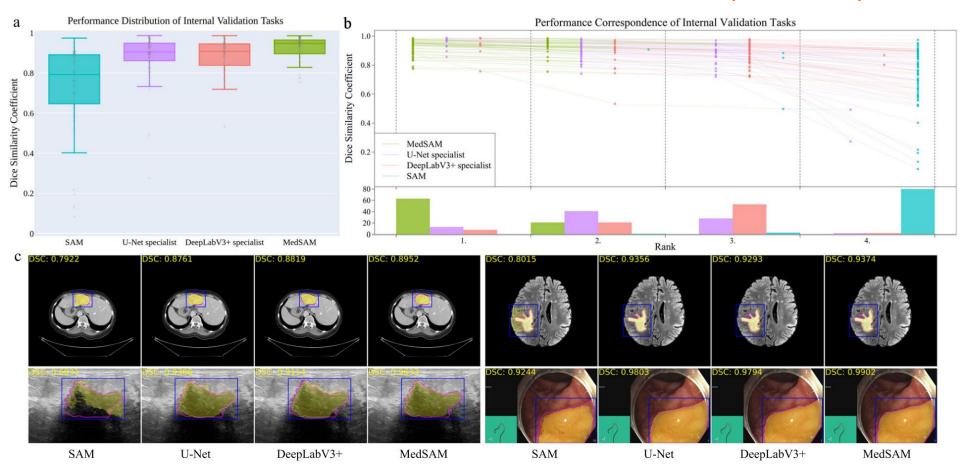
Dice similarity coefficient: evaluate the region overlap between expert annotation masks and segmentation results

$$ext{NSD}(G,\,S) \,=\, rac{|\partial G \cap B_{\partial S}^{(au)}| + |\partial S \cap B_{\partial G}^{(au)}|}{|\partial G| + |\partial S|}$$

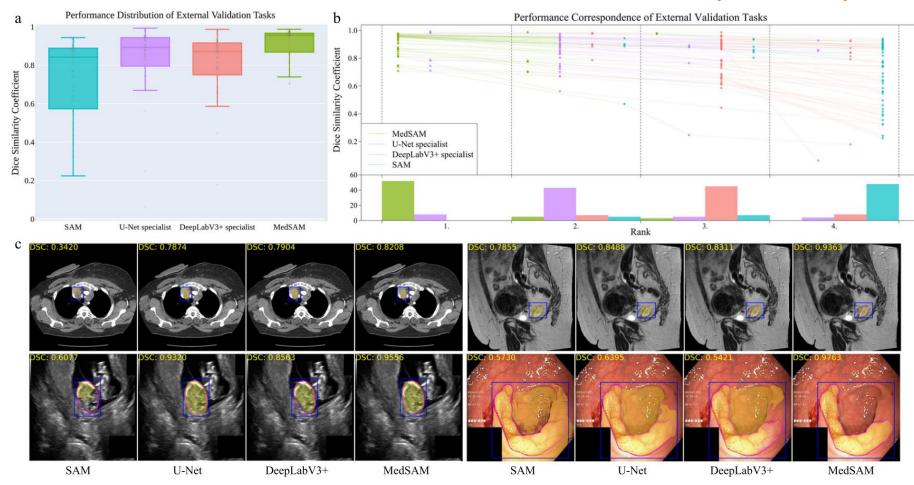
Normalized surface distance: evaluate the boundary consensus between expert annotation masks and segmentation results at a given tolerance

where $B_{\partial G}^{(\tau)}=\{x\in R^3\mid \exists ilde{x}\in\partial G,\ ||x- ilde{x}||\leq au\}$, $B_{\partial S}^{(\tau)}=\{x\in R^3\mid \exists ilde{x}\in\partial S,\ ||x- ilde{x}||\leq au\}$ denote the border region of the expert annotation mask and the segmentation surface at tolerance au, respectively. In this paper, we set the tolerance au as 2.

Performance distribution of 86 internal validation tasks (DSC score)



Performance distribution of 60 external validation tasks (DSC score)



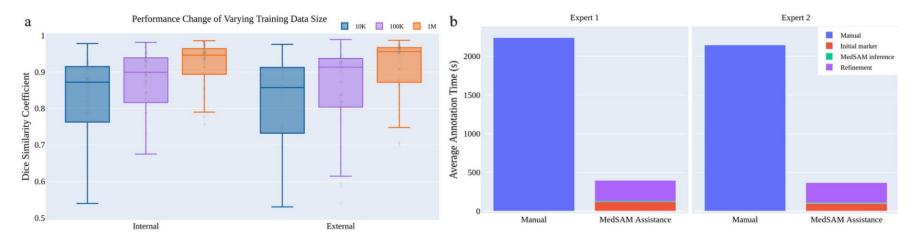


Fig. 5 | **The effect of training dataset size and a user study of tumor annotation efficiency. a** Scaling up the training image size to one million can significantly improve the model performance on both internal and external validation sets.

b MedSAM can be used to substantially reduce the annotation time cost. Source data are provided as a Source Data file.

- Linear marker every 3-10 slices by two experts, before MedSAM segmentation, and expert revision (3D adrenal tumors)
- Annotation time reduced by 82.37% and 82.95% for the two experts respectively

Some external validation on MRIs (DSC and NSD)



Fig. 11. Box plots of dice similarity coefficient and normalized surface distance scores for each MR segmentation task in external validation. The center line within the box represents the median value, with the bottom and top bounds of the box delineating the 25th and 75th percentiles, respectively. Whiskers are chosen to show the 1.5 of the interquartile range. Source data are provided as a Source Data file.

Discussion

Limitations:

- Modality imbalance in the training set: underperform on less-represented modalities
- Bounding box prompt can be ambiguous for segmentation of vessel-like branching structures

Conclusion:

Holds great potential to accelerate the advancement of new diagnostic and therapeutic tools



Discussion