## MODEL-BASED SUPER-RESOLUTION RECONSTRUCTION OF T2 MAPS

Wajiha Bano<sup>1,2</sup>, Gian Franco Piredda<sup>3,4,5</sup>, Mike Davies<sup>1</sup>, Ian Marshall<sup>2</sup>, Tobias Kober<sup>3,4,5</sup>, Jean-Philippe Thiran<sup>4,5</sup>, Tom Hilbert<sup>3,4,5</sup>

<sup>1</sup>Institute for Digital Communications, University of Edinburgh, Edinburgh, UK. <sup>2</sup>Centre for Clinical Brain Sciences, University of Edinburgh, Edinburgh, UK. <sup>3</sup> Advanced Clinical Imaging Technology, Siemens Healthcare AG, Lausanne, Switzerland. <sup>4</sup> LTS5, École Polytechnique Fédérale de Lausanne, Lausanne, Switzerland. <sup>5</sup> Department of Radiology, University Hospital Lausanne (CHUV), Switzerland

Introduction: High-resolution isotropic T2 mapping of human brain with multi-echo spin-echo acquisitions (MESE) is difficult due to the slice thickness limitation of a 2D sequence. Furthermore, if used as a 3D acquisition, SAR limits are easily exceeded due to the high power deposition of nonselective refocusing pulses. Here, we propose a method to reconstruct 1-mm<sup>3</sup> isotropic T2 maps based on multiple 2D MESE acquisitions. To compensate for the prolonged scan time due to multiple acquisitions, data were highly (10-fold) undersampled.

Methods: Data from a multipurpose phantom and four healthy subjects were acquired at 3T (MAGNETOM Skyra, Siemens Healthcare, Erlangen, Germany) with a 10-fold accelerated GRAPPATINI prototype sequence (1). (60 slices, (1x1x4) mm<sup>3</sup> resolution, (256x240x240) mm<sup>3</sup> FOV, TR=5.4s, ΔTE=10ms, ETL=16, TA=4:31min). The acquisition was repeated four times, and for each scan, the FOV was rotated in 45° steps about the longitudinal axis (total TA=18:04min). The reconstruction integrated super-resolution (SR) (2) and model-based (3) approaches (see Eq. 1). A high-resolution image  $x_n$  was estimated by minimizing the difference to LR k-space  $y_{n,c}$  with  $S_c$  coil sensitivities, T four 45° rotations, \( \) downsampling to LR grid, F Fourier transform and P undersampling. Next, the image corresponding to the signal-model  $\hat{x}_n = M_0 exp(-\frac{TE}{T2})$  was calculated by fitting a monoexponential decay onto  $x_n$ , intrinsically estimating T2 and M0. The weighting factor  $\lambda$  balanced data and model consistency.

$$\underset{T2,M_{0},x_{n}}{argmin} \sum_{n}^{N} \sum_{c}^{C} \| PF \{ \downarrow TS_{c}x_{n} \} - y_{n,c} \|^{2} + \lambda \| x_{n} - \hat{x}_{n} \|^{2}$$
 (1)

Fully sampled MESE images were acquired for comparison.

Results: High-resolution isotropic T2 maps from the phantom and one subject are shown in Fig.1. In comparison with the fully sampled acquisition, the SRreconstructed images demonstrated resolution improved in all three dimensions (see also Fig. 2).

Conclusion: The proposed method shows feasibility for high-resolution relaxometry based on acquisition which may enable its wide application in studying small brain structures and changes in their physical properties

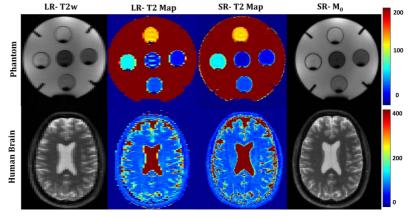


Figure 1: LR T2w images, LR T2 map, SR T2 maps and *M*<sub>0</sub> reconstructed for phantom (top row) and human brain (bottom row). The colorbar represents T2 values in ms.

References: 1. Greenspan et al. MRI 2003. 2. Hilbert et al. JMRI 2018. 3. Bano et al. ISMRM 2018.

Figure 2: Axial and Coronal view of T2-weighted images reconstructed with SR-T2 mapping and fully sampled MESE images. Zoomed-in images depict the better resolution in both planes for SR volumes as compared to conventional sequence.

## SR- T2 Mapping

**MESE- T2 Mapping** 

## **Acknowledgements:**

The research leading to these results has received funding from the European Union's Seventh Framework Programme (FP7-PEOPLE-2013-ITN) under grant agreement n 607290 SpaRTaN.

Coronal