

From Static to Fast Transient Dynamic Brain Networks

Diego Vidaurre

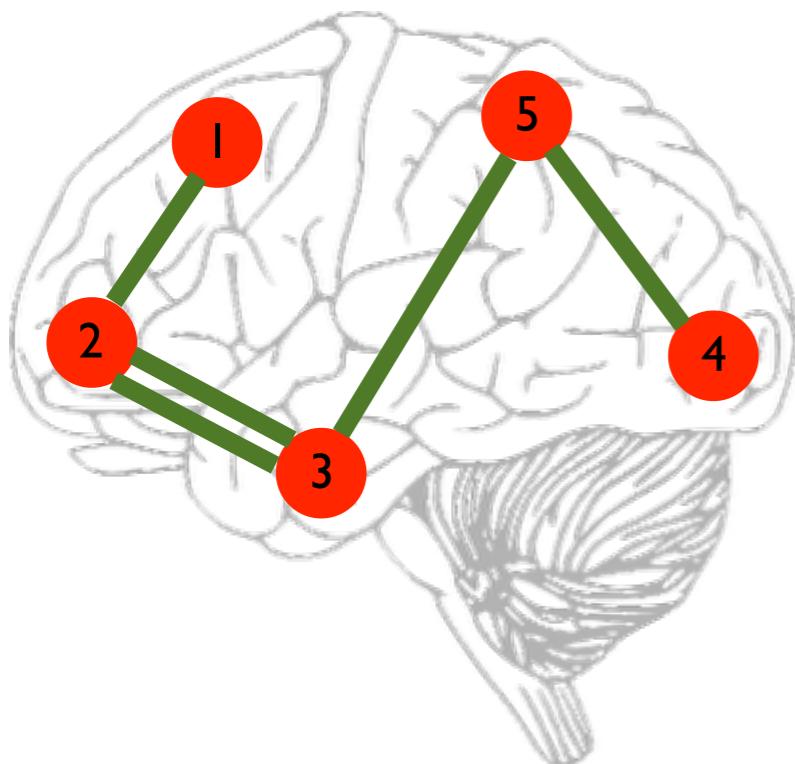
Department of Psychiatry

University of Oxford

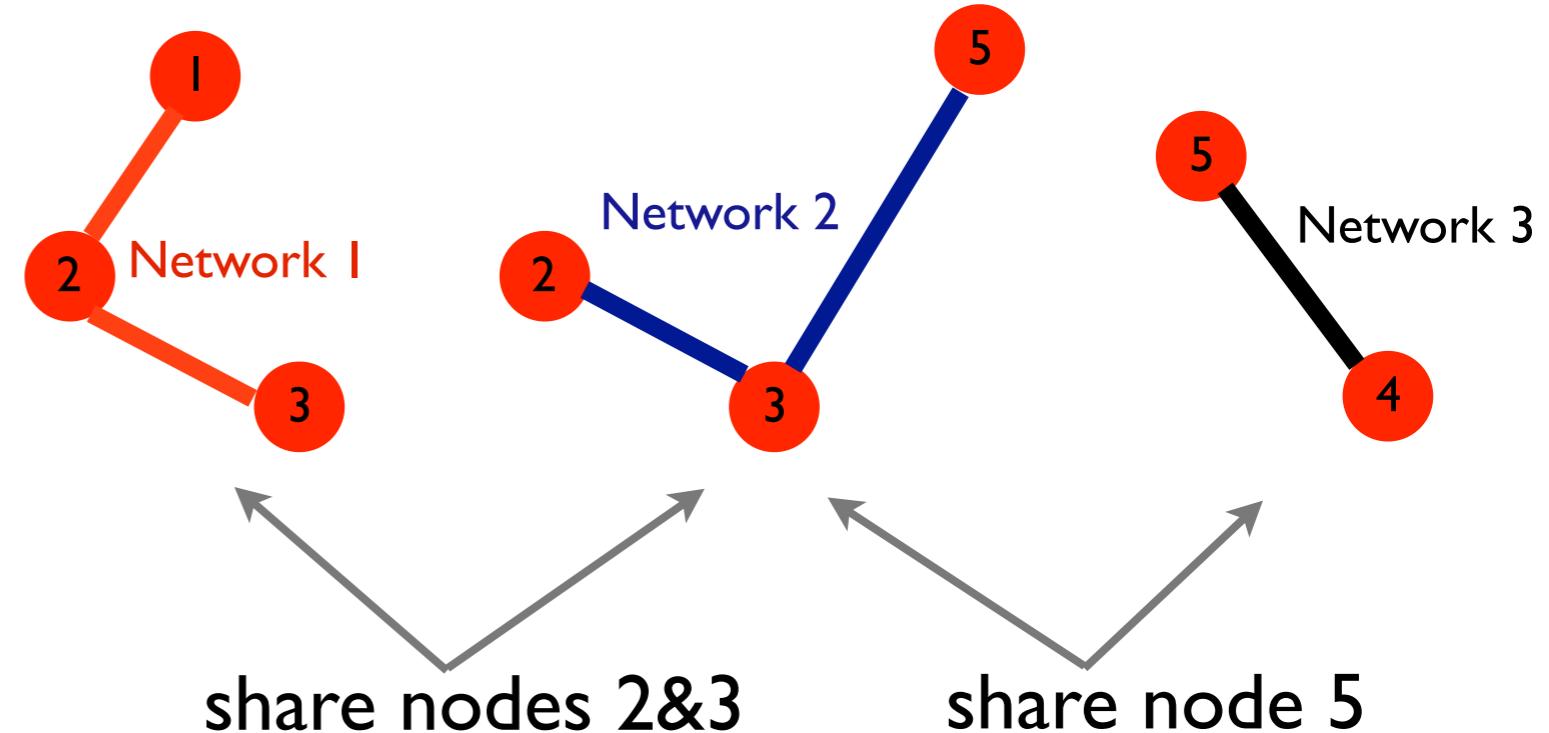
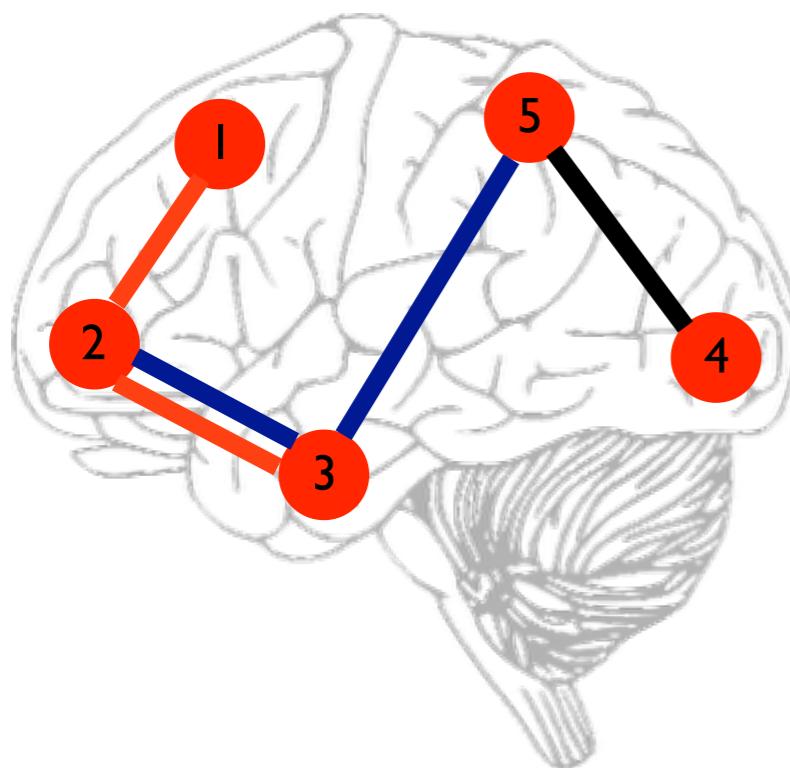


Oxford centre for Human Brain Activity

Resting state network



Resting state network



Network 1, 2 and 3 have distinct spatial and temporal characteristics that could not have been found in a static analysis

Goals

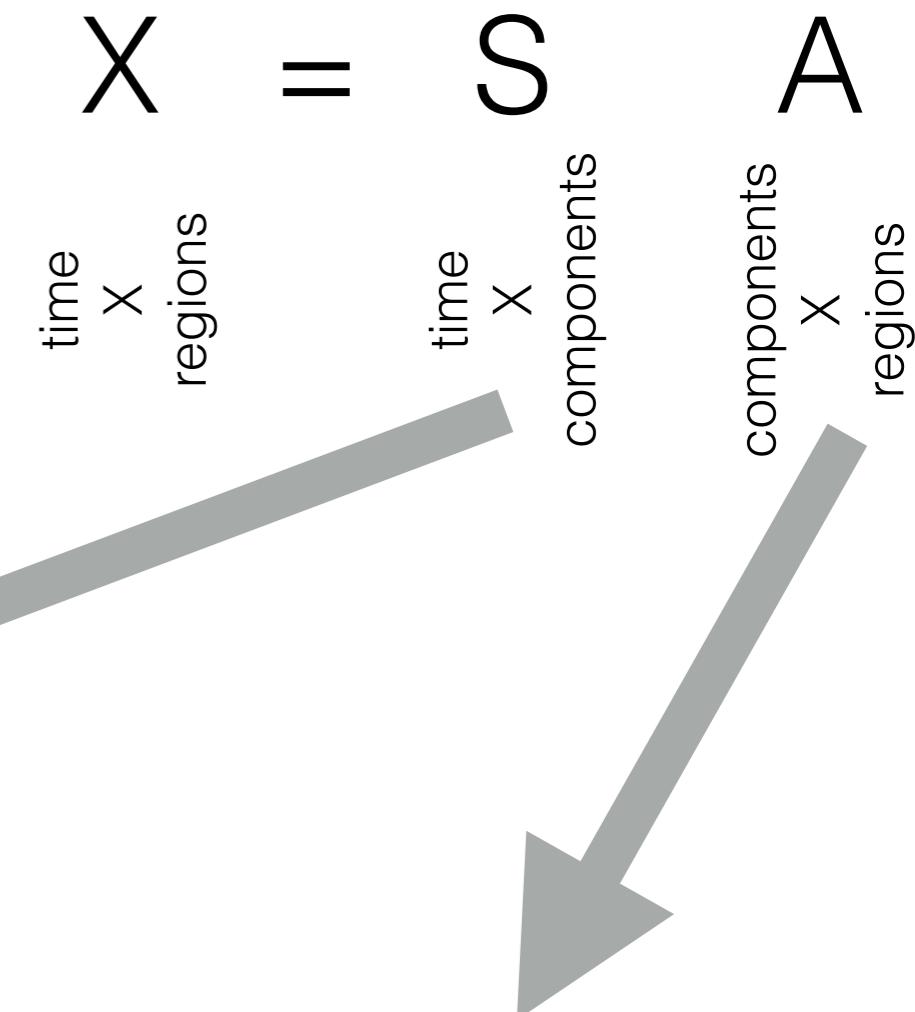
- What is happening at **faster** time-scales?
- What are the specific temporal interactions, or network dynamics?
- How activity organises temporally and spatially in rest, and how connectivity is modulated in task

Can we use MEG to answer these questions?

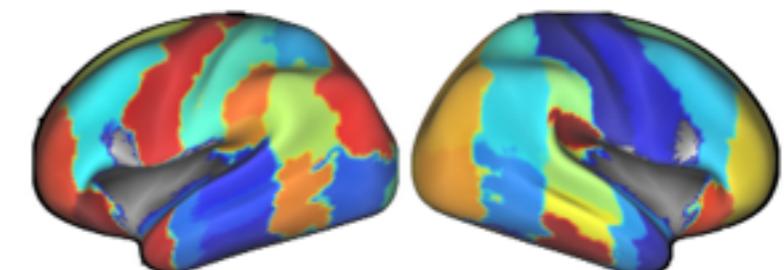
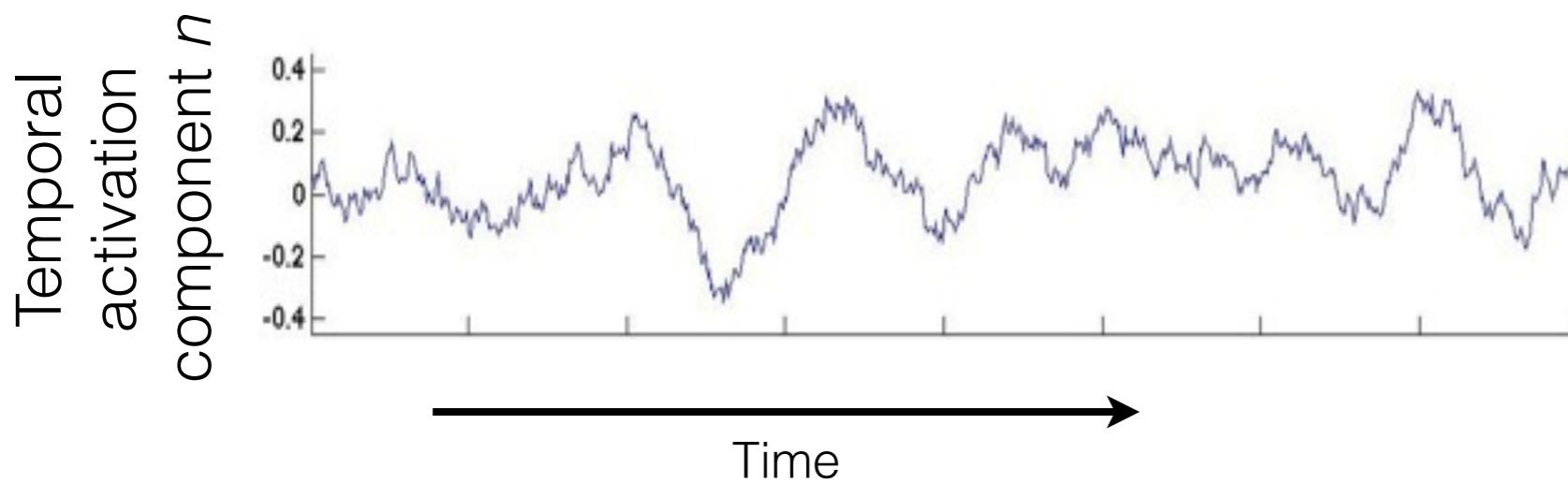


Temporal Independent Component Analysis

- Activation pattern or components (A)
- Component time courses (S)
- Specified on power time series 
- Components do not reflect functional connectivity



Spatial activation component n

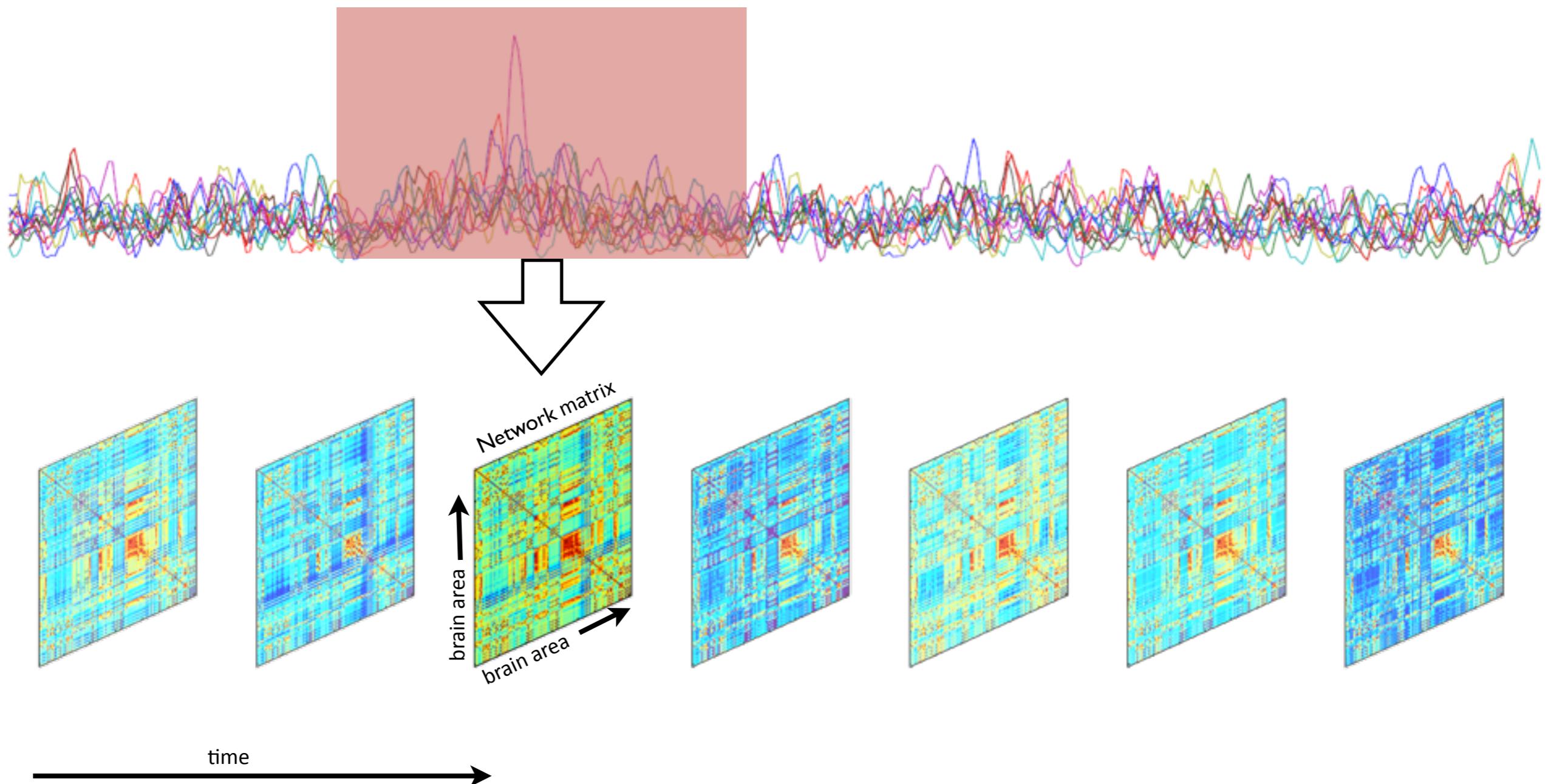


Brookes et al (PNAS 2011)

State-of-the-art methods: Sliding Windows

Compute **sliding window** correlation network matrices

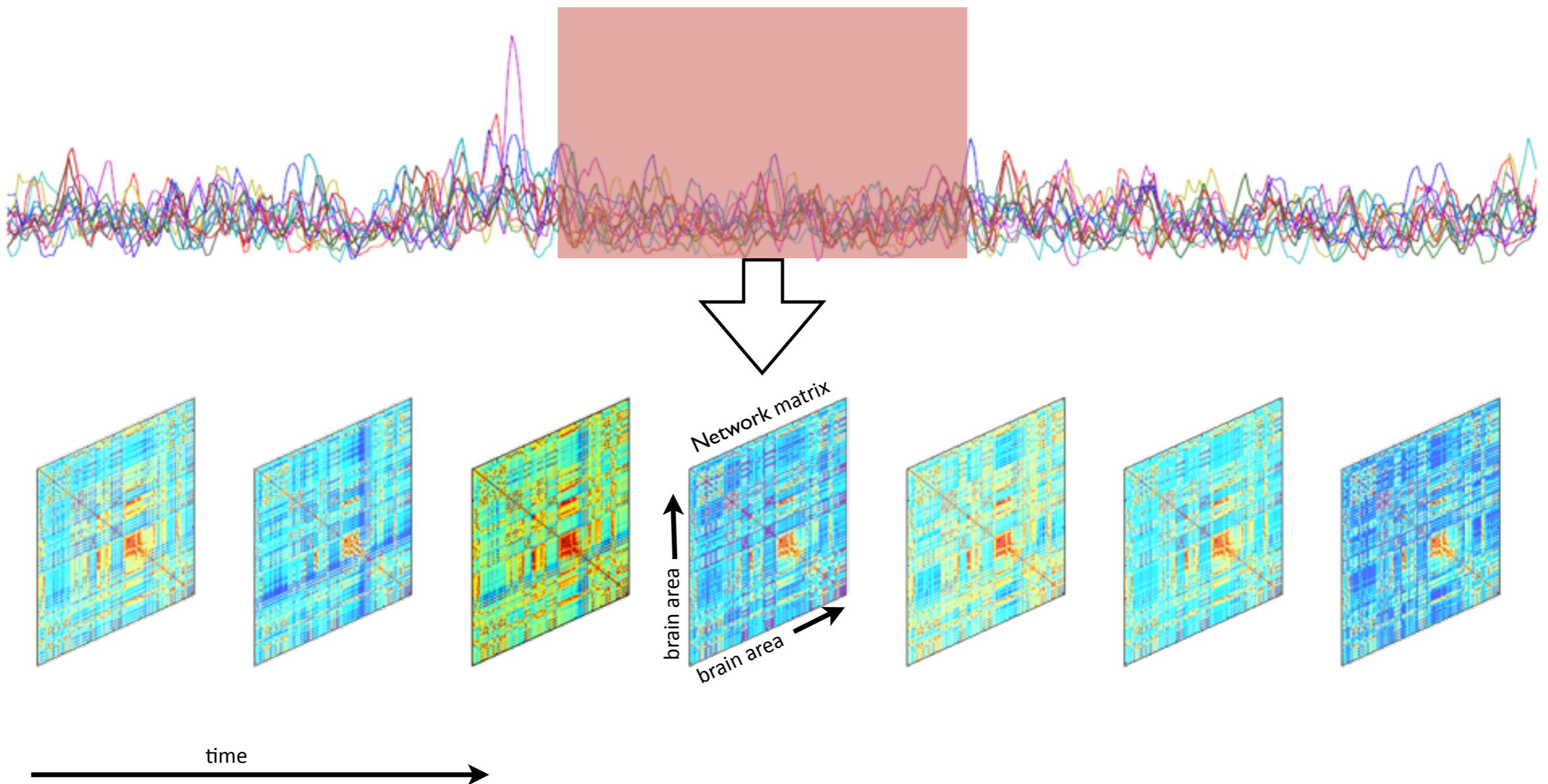
Sliding window (~1sec)



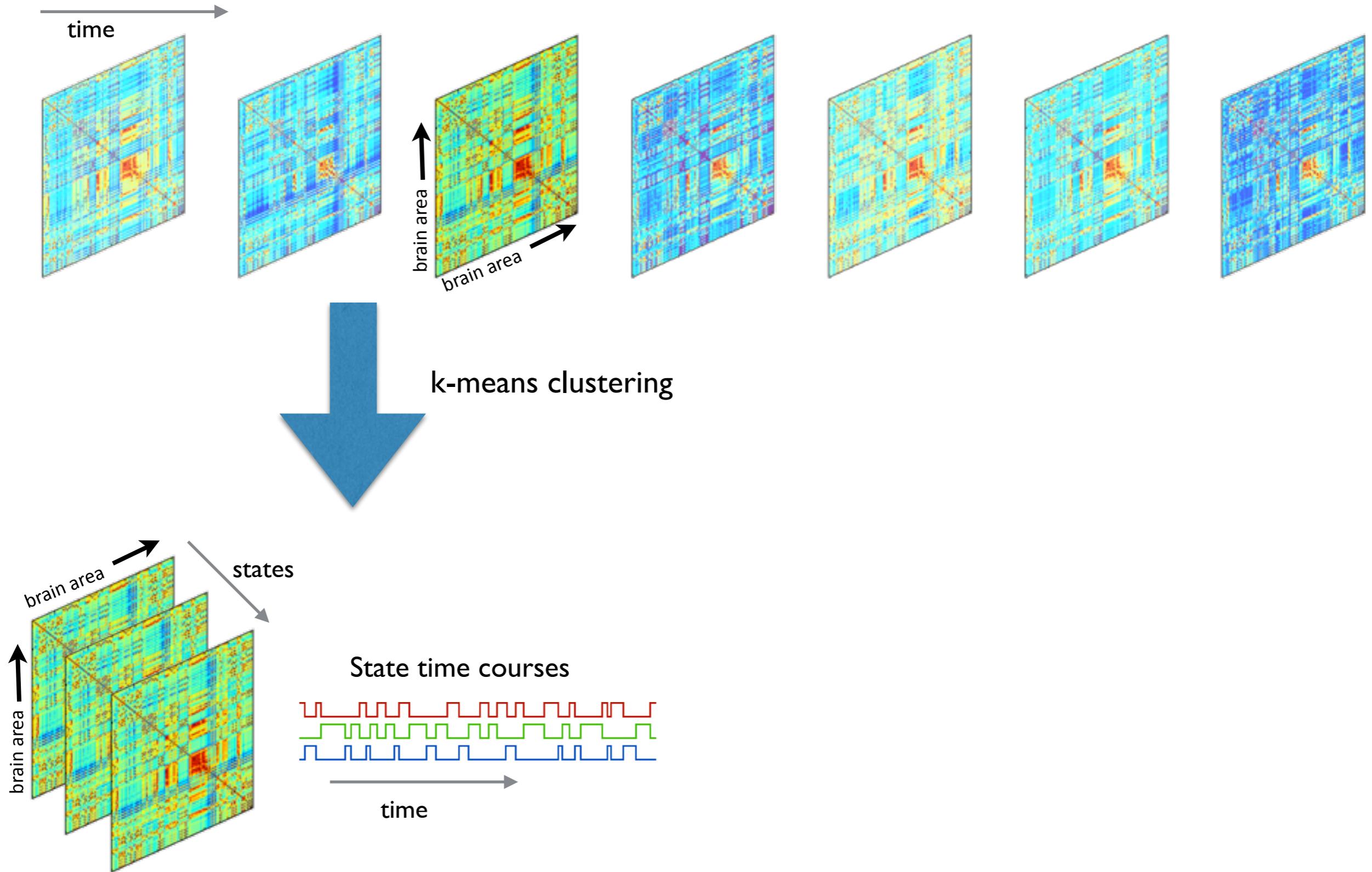
State-of-the-art methods: Sliding Windows

Compute **sliding window** correlation network matrices

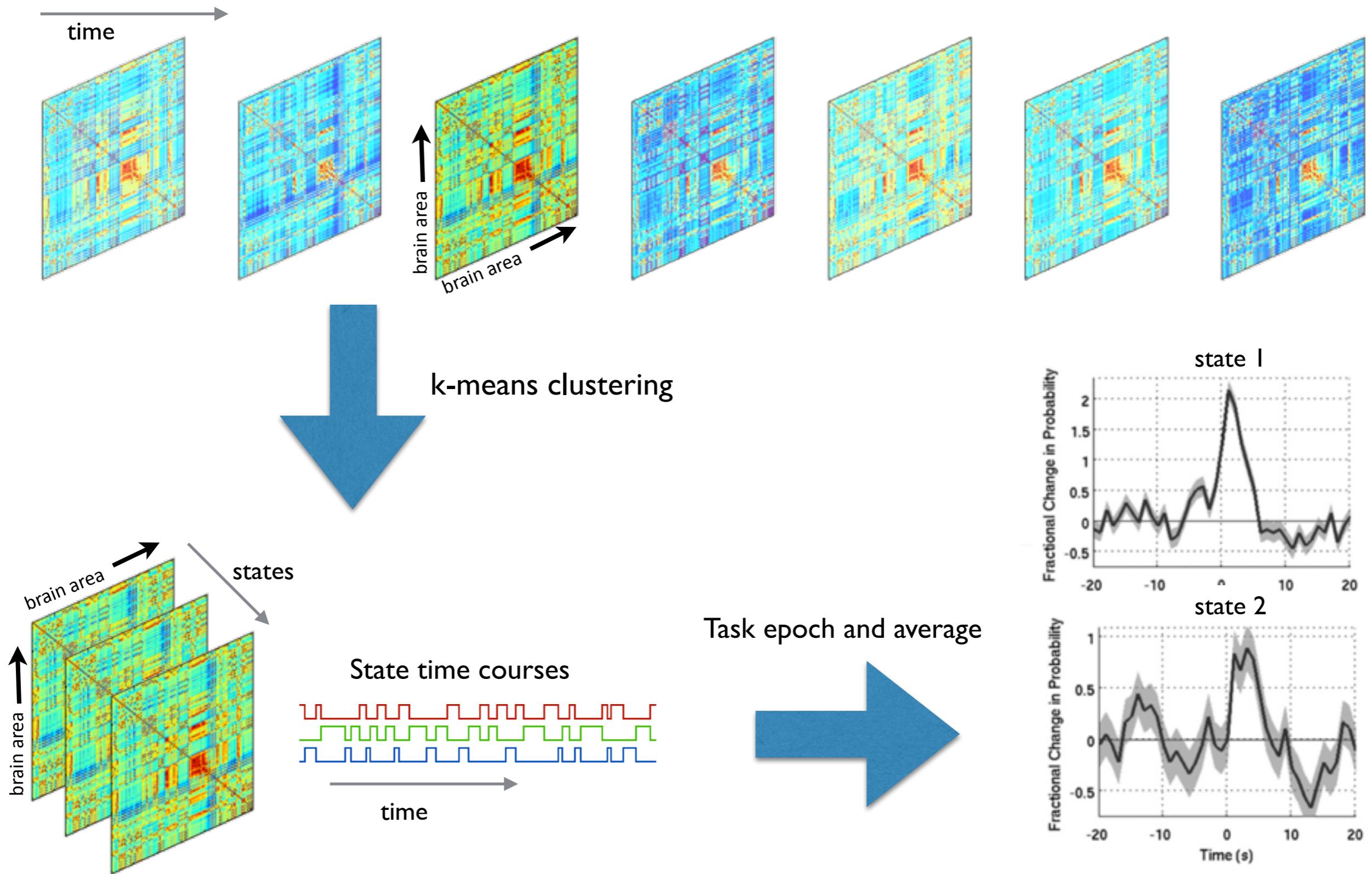
Sliding window (~1sec)



State-of-the-art methods: Sliding Windows



State-of-the-art methods: Sliding Windows



Issues:

How to choose the width of the window?

- too short - unstable, unreliable estimation
- too long - misses quick changes

Inefficient use of the data

- No matter how much data we have, each estimation is based on a small portion of the data



Can sliding-window correlations reveal dynamic functional connectivity in resting-state fMRI?

R. Hindriks ^{a,*}, M.H. Adhikari ^a, Y. Murayama ^d, M. Ganzetti ^{b,c}, D. Mantini ^{b,c}, N.K. Logothetis ^d, G. Deco ^{a,e}

^a Center for Brain and Cognition, Computational Neuroscience Group, Department of Information and Communication Technologies, Universitat Pompeu Fabra, Barcelona, Spain

^b Department of Health Sciences and Technology, ETH Zurich, Switzerland

^c Department of Experimental Psychology, University of Oxford, United Kingdom

^d Department of Physiology of Cognitive Processes, Max Planck Institute for Biological Cybernetics, Tübingen, Germany

^e Institut Català de la Recerca i Estudis Avançats (ICREA), Universitat Pompeu Fabra, Barcelona, Spain

ORIGINAL ARTICLE

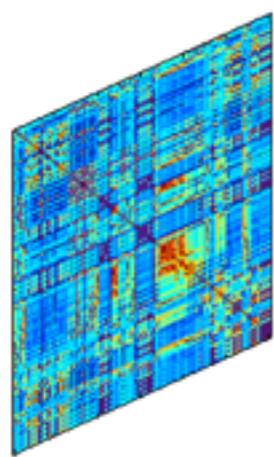
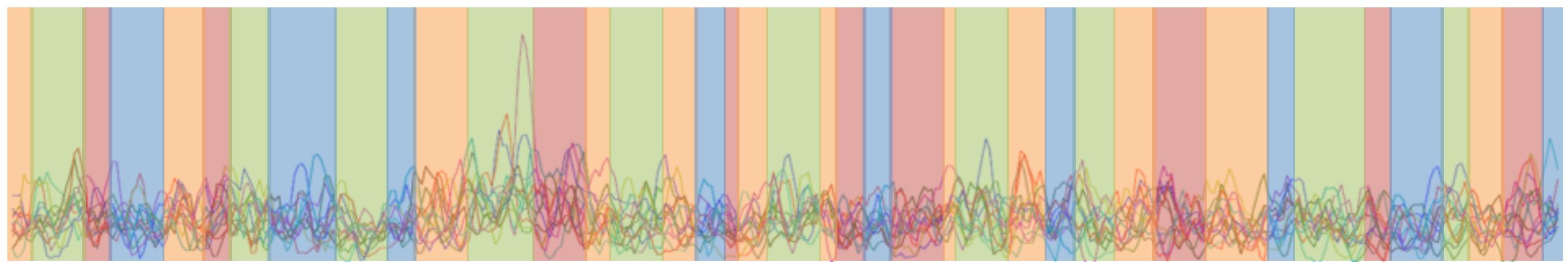
Cerebral CORTEX

On the Stability of BOLD fMRI Correlations

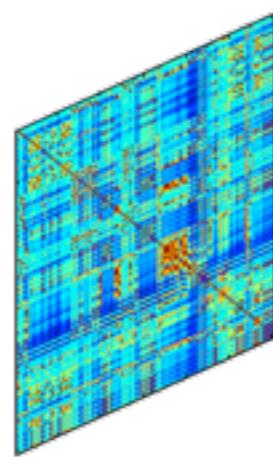
Timothy O. Laumann¹, Abraham Z. Snyder^{1,2}, Anish Mitra², Evan M. Gordon^{3,4}, Caterina Gratton¹, Babatunde Adeyemo¹, Adrian W. Gilmore⁵, Steven M. Nelson^{3,4}, Jeff J. Berg⁵, Deanna J. Greene^{2,6}, John E. McCarthy⁷, Enzo Tagliazucchi^{8,9}, Helmut Laufs^{9,10}, Bradley L. Schlaggar^{1,2,6,11,12}, Nico U. F. Dosenbach¹, and Steven E. Petersen^{1,2,5,12}

Hidden Markov Model

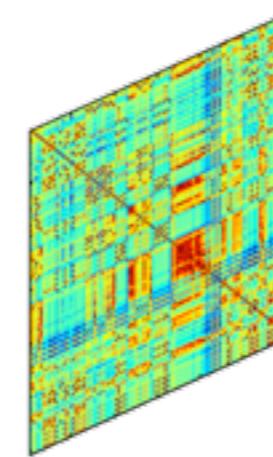
Instead pool data over disjoint time periods:



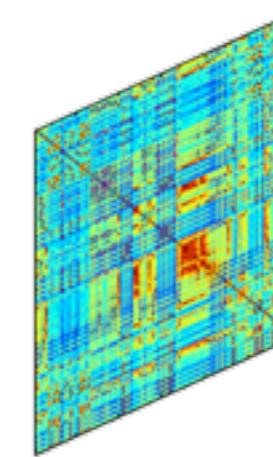
State 1



State 2



State 3



State 4

Fundamental assumptions

- One state is assumed at a time although we effectively estimate the probability of each state being active at each time point t
- Which state is active at time t depends on which state was active at time point $t-1$ which means that the influence of the past decreases exponentially

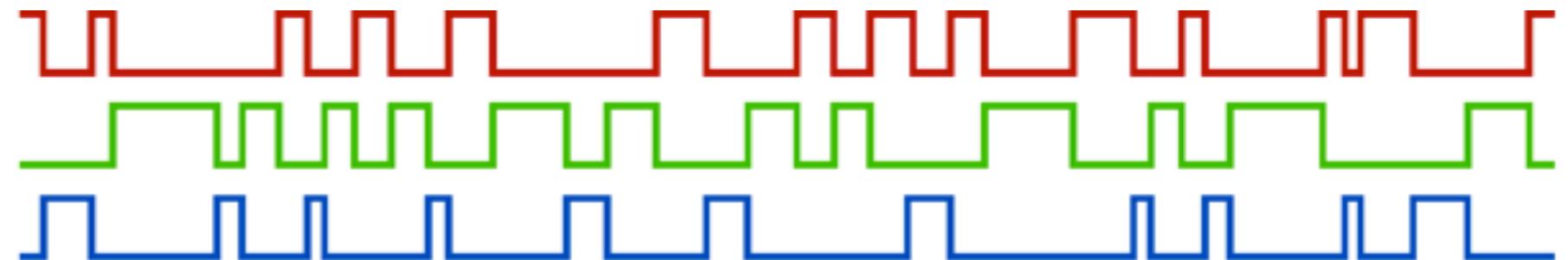
Benefits

- We do not need to specify the window length
- We make an efficient use of the data
- We can access the fastest time scales

Hidden Markov Model

State time courses:

When

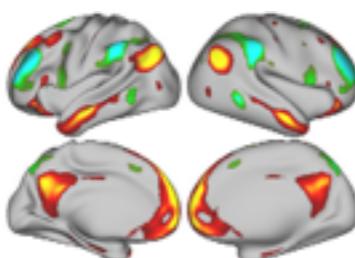


State probability distribution

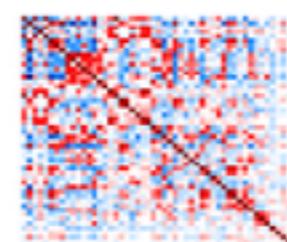
(one for each state):

What

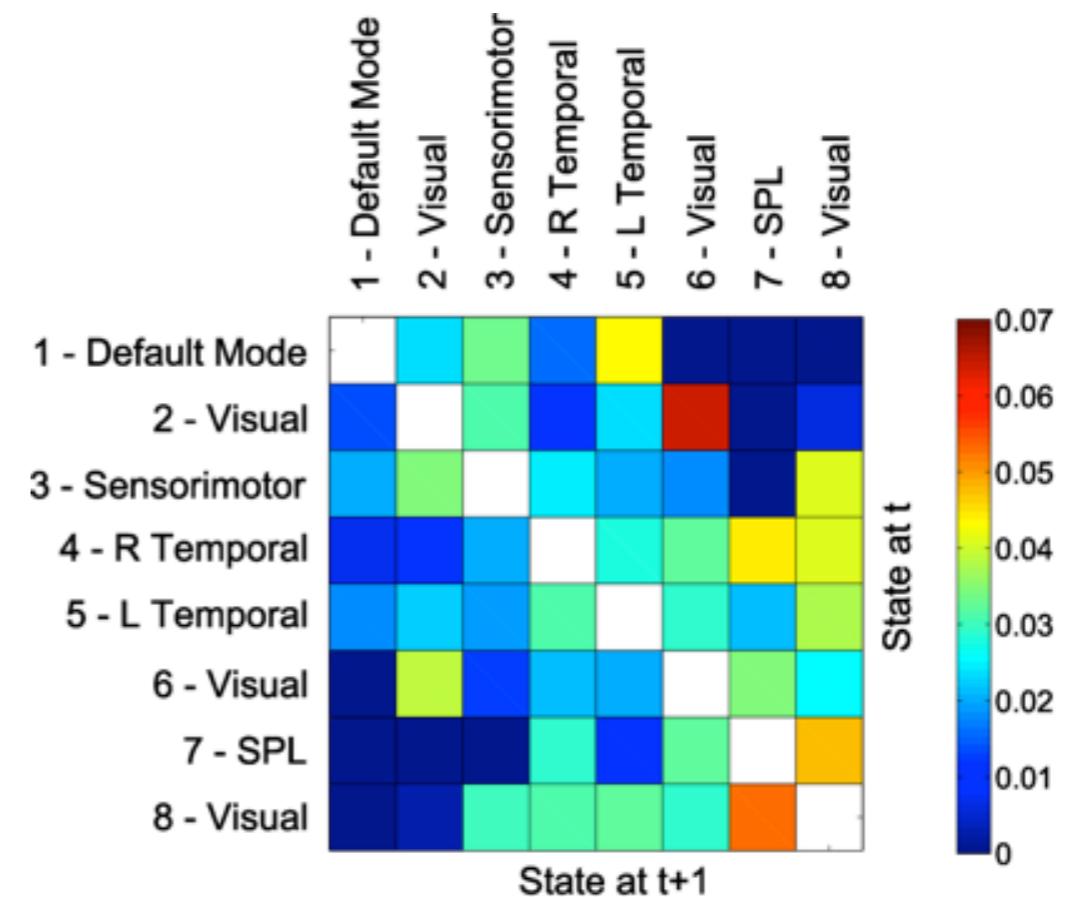
Mean activation



Functional connectivity



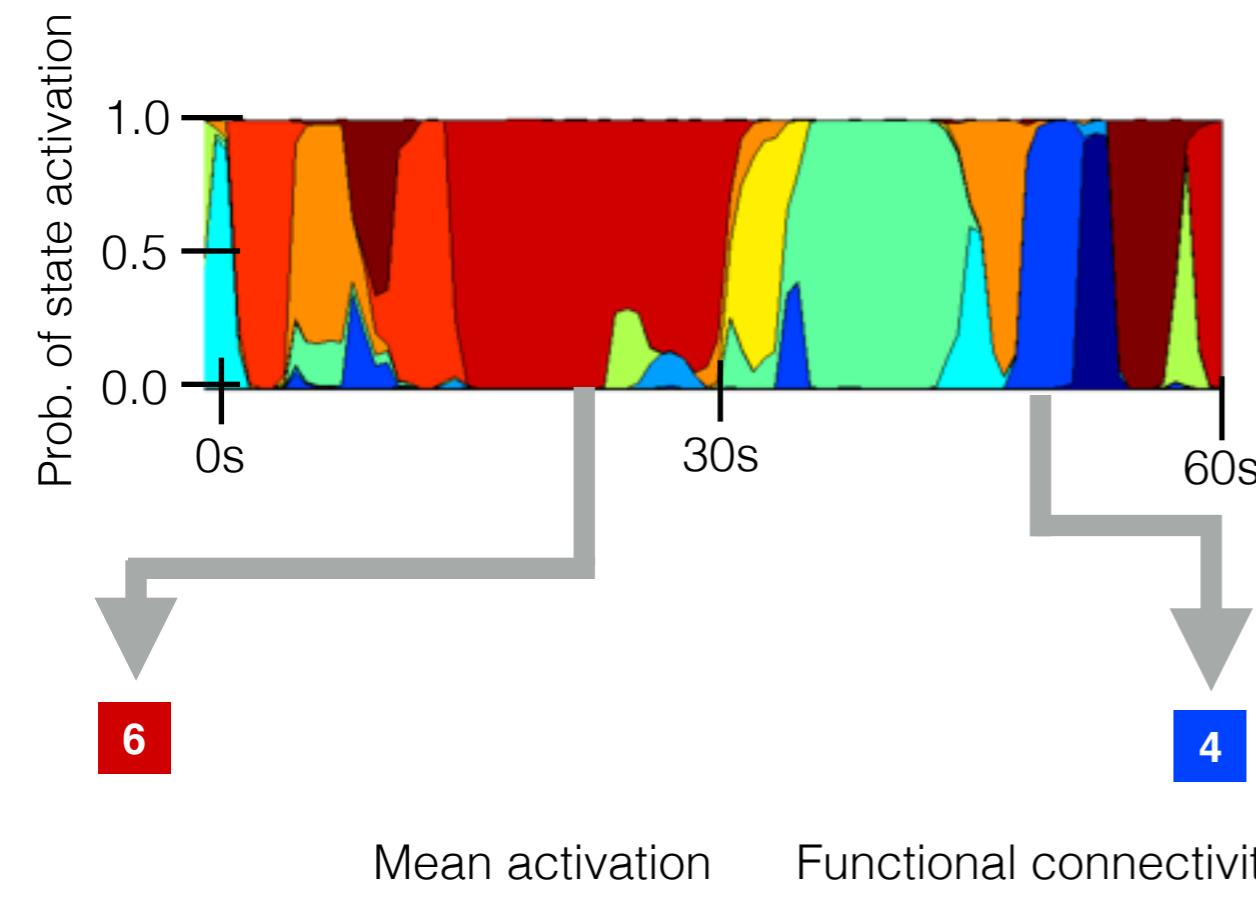
*Different classes of probability distributions adapt
to different classes of data
this is a user choice*



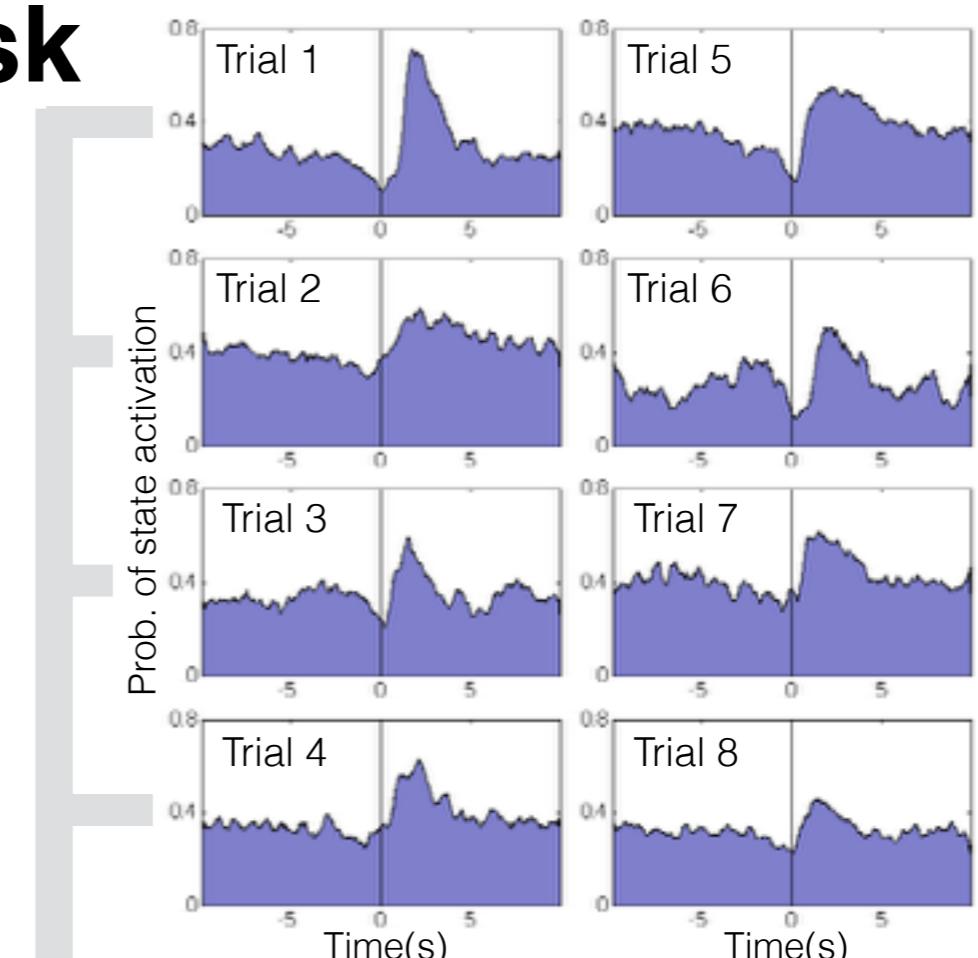
**Transition probability
matrix**

Hidden Markov Model

In rest

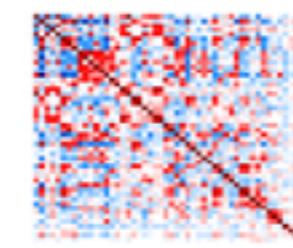
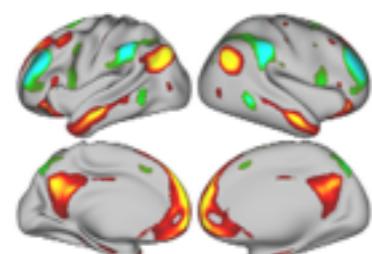


In task



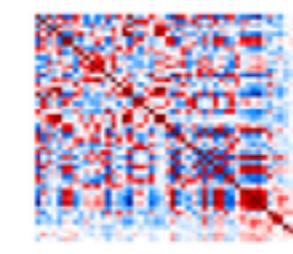
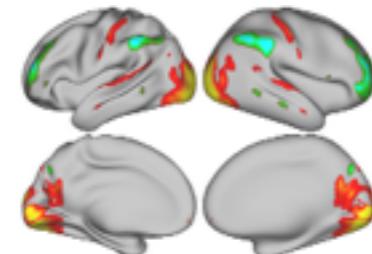
6

DMN

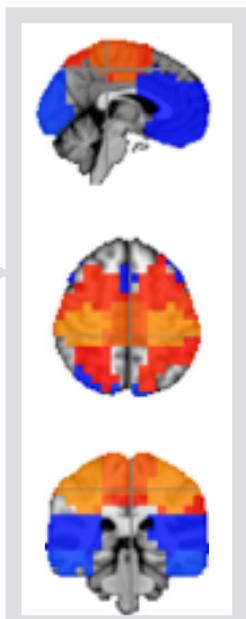
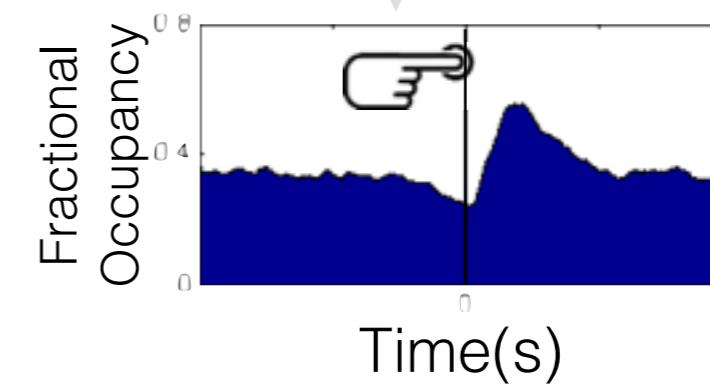


4

Visual network



Average



Hidden Markov Model

At the group level

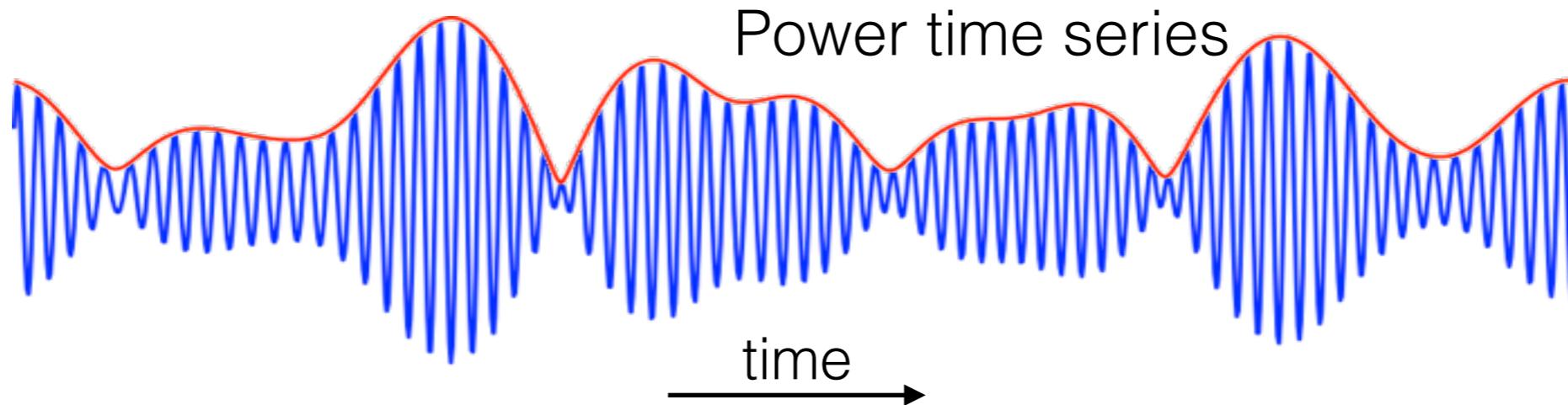


At the subject level

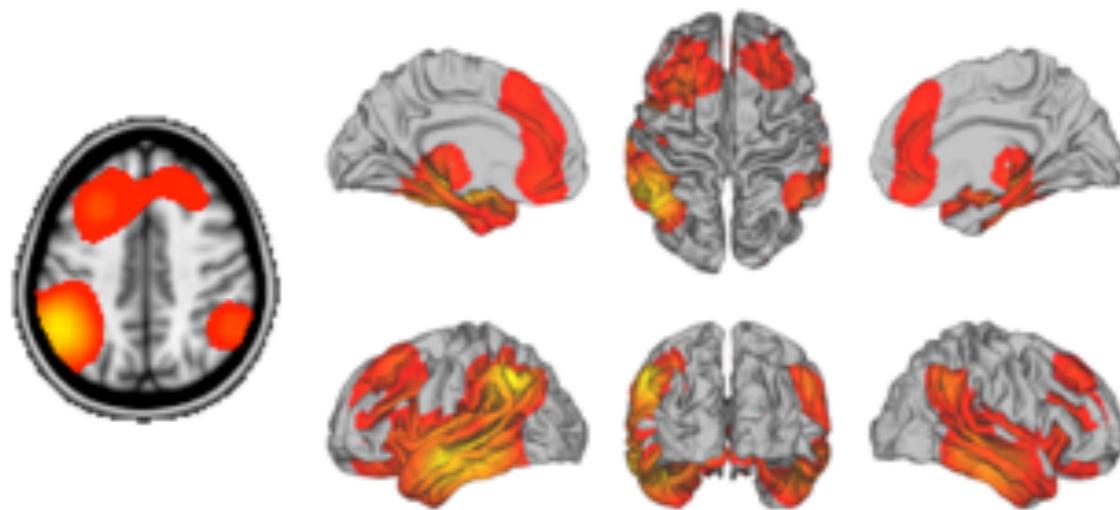


HMM-Gaussian

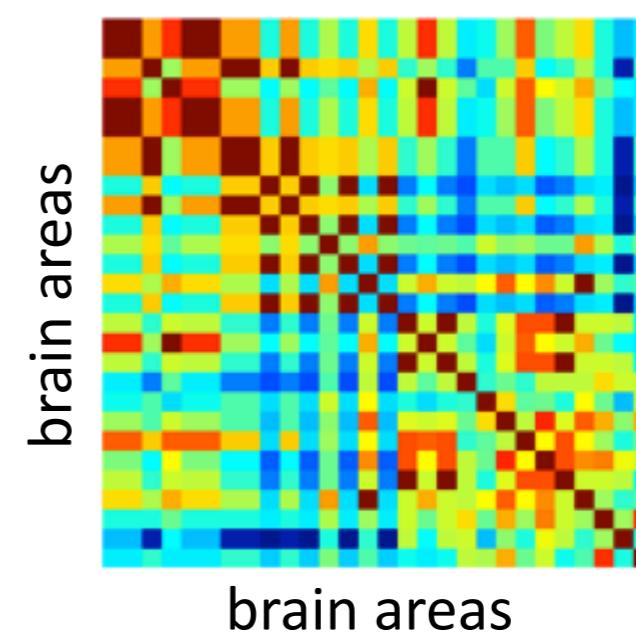
What is a brain state? A Gaussian distribution $\mathcal{N}(\mu, \Sigma)$



Mean activation μ

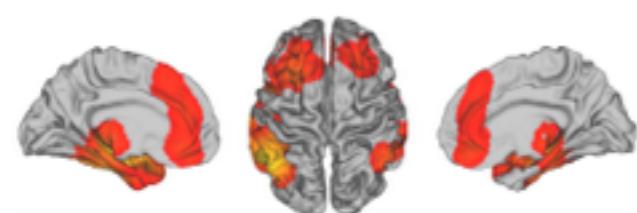


Network matrix Σ
(power correlation)

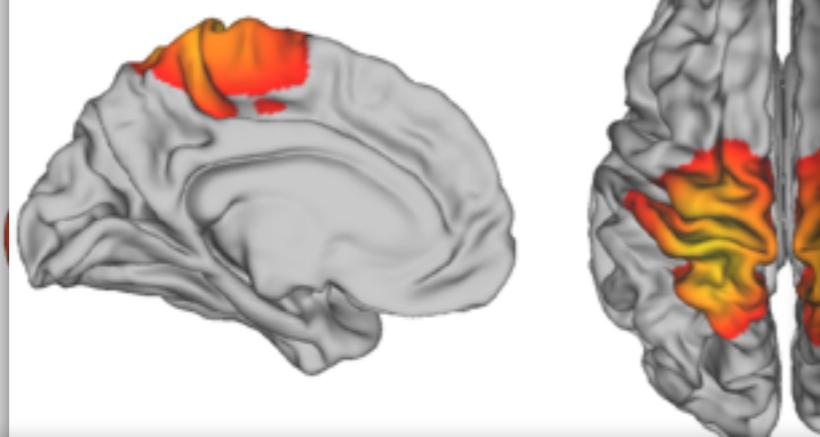


HMM-Gaussian

State 1
DMN

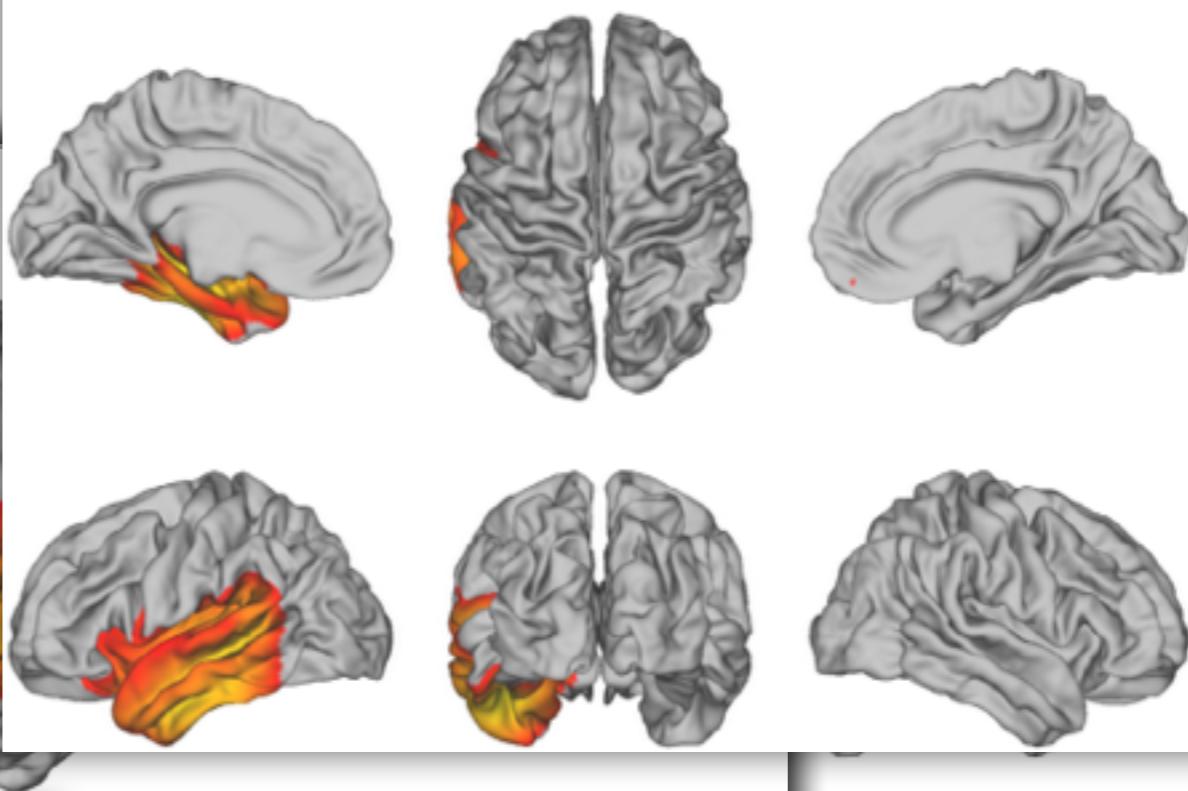


State 3

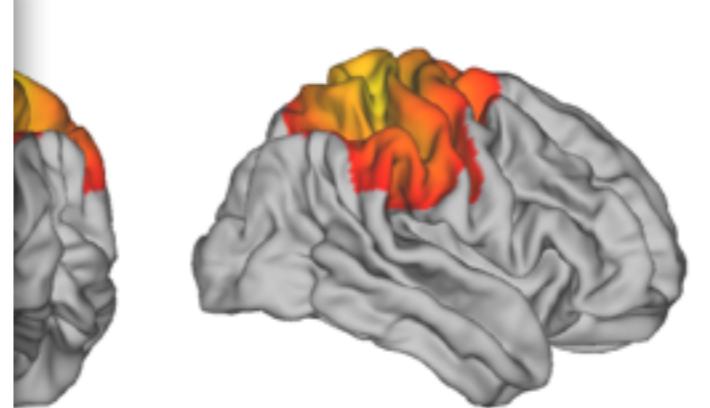
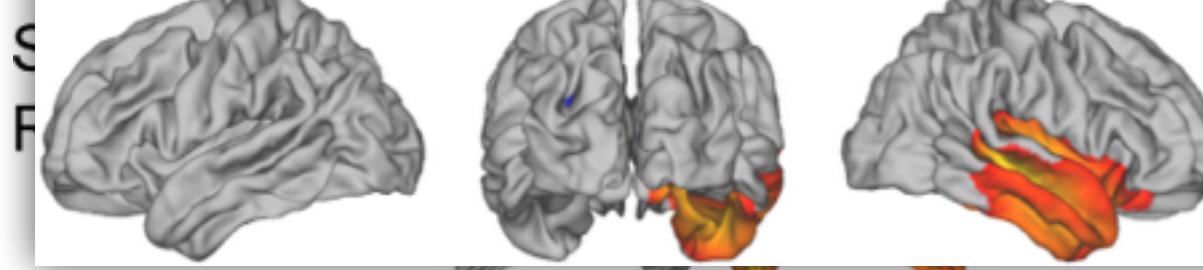
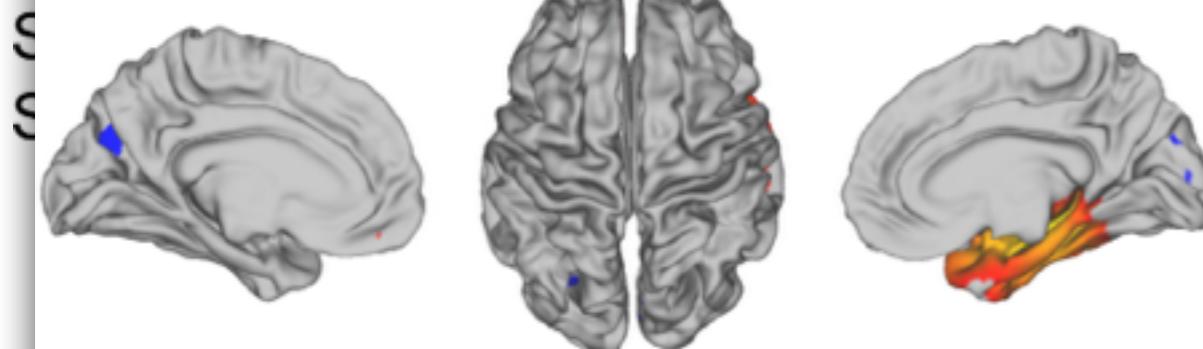


State 2
Visual

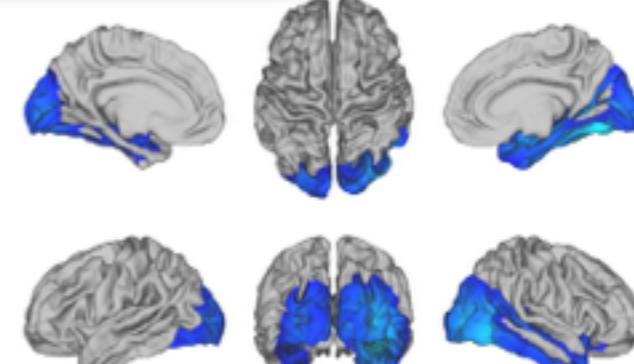
State 5



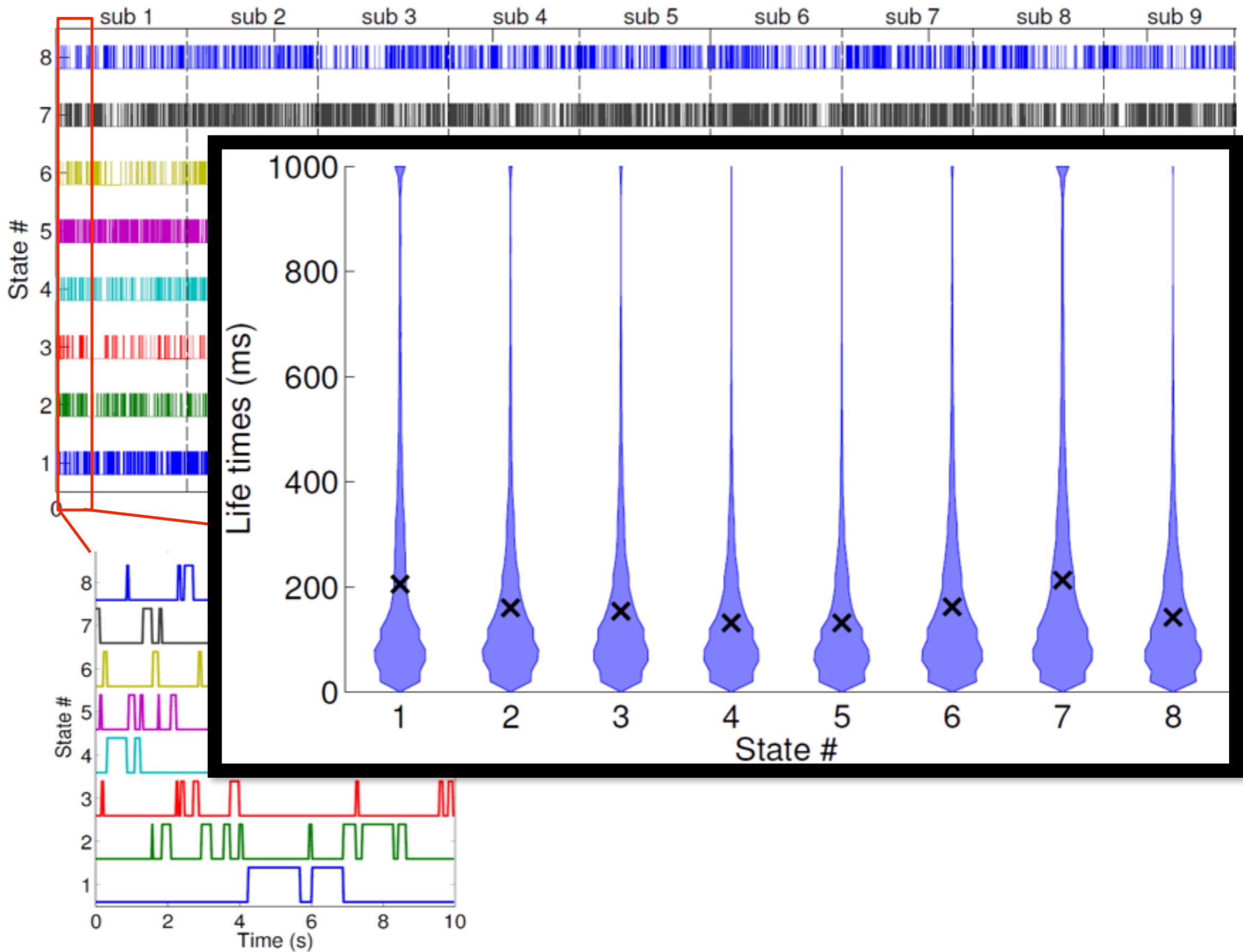
State 4



State 8
Visual



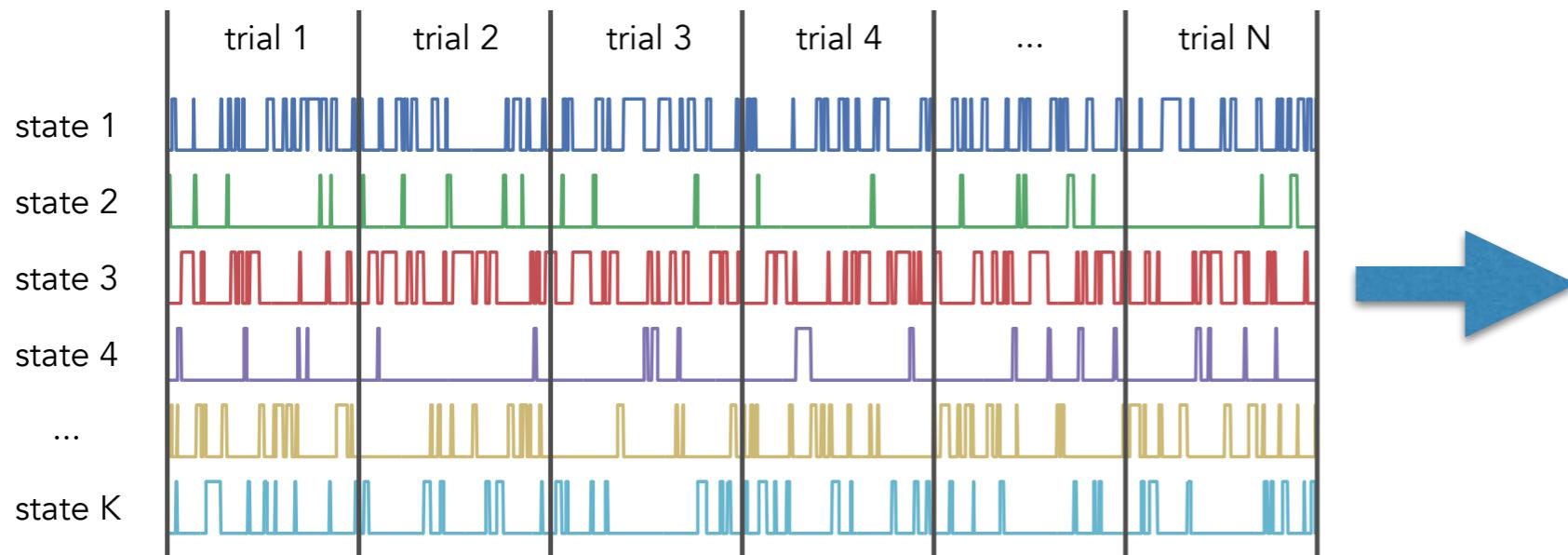
HMM-Gaussian



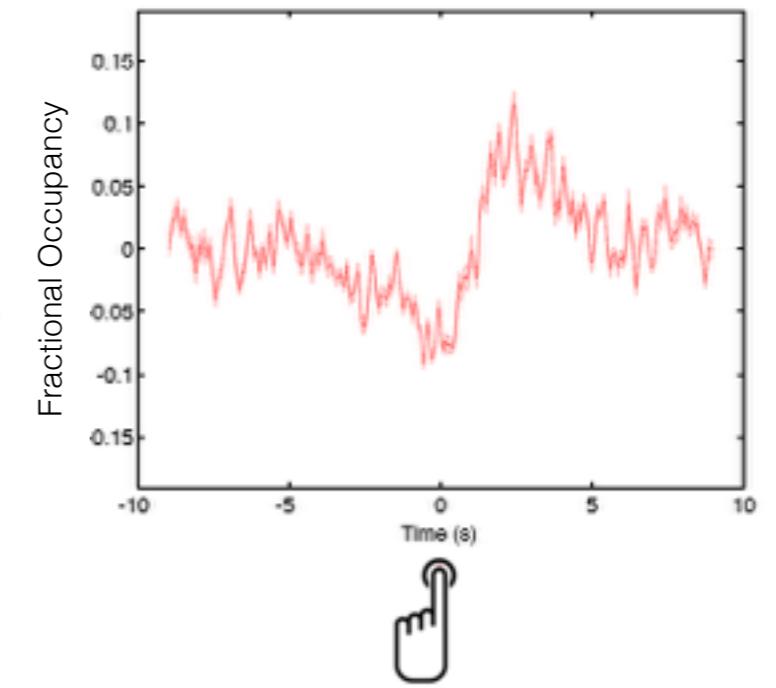
TASK DATA

- Fit HMM to task data, **then** epoch and average the state time courses over trials

HMM state time courses

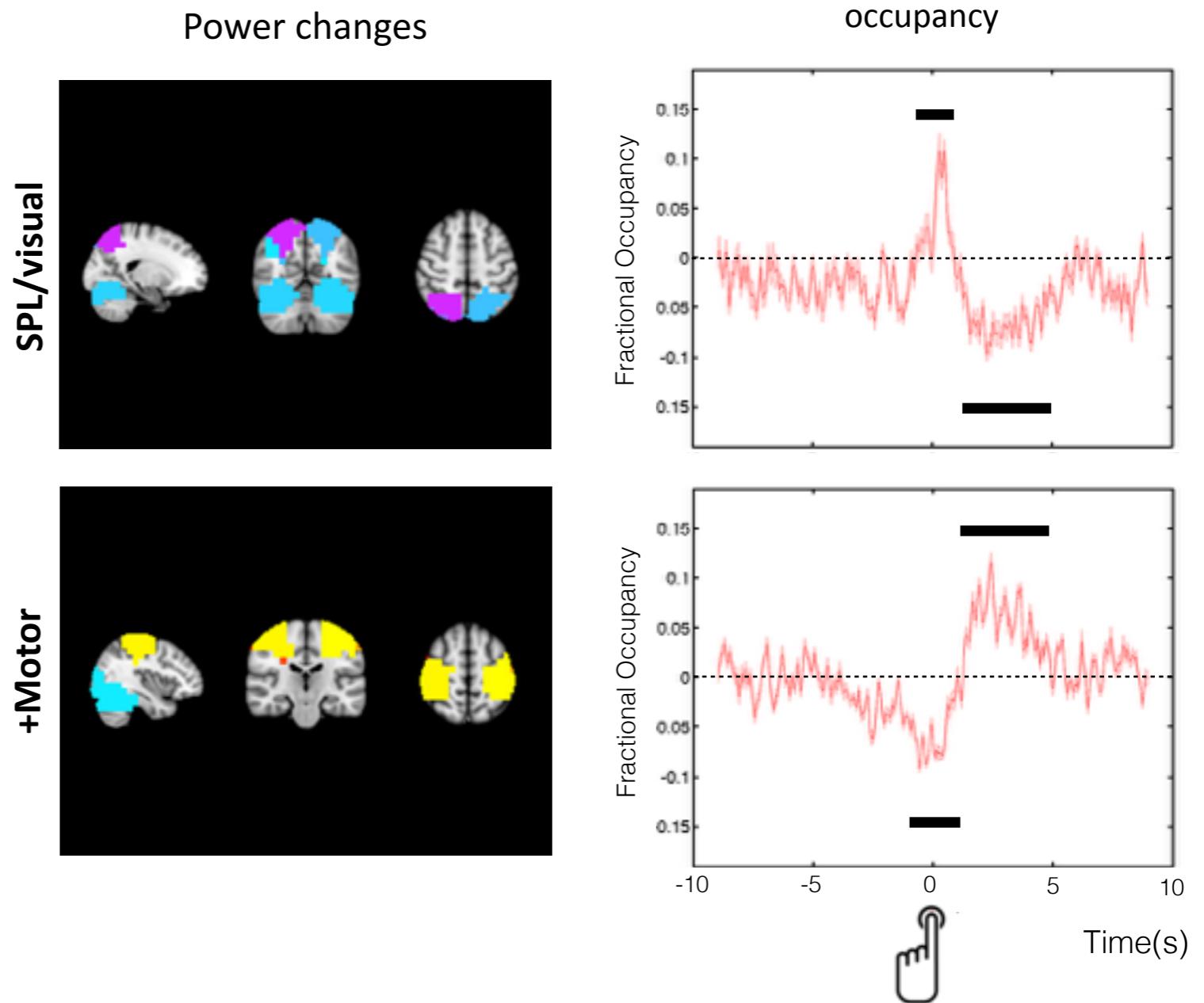


Fractional Occupancy



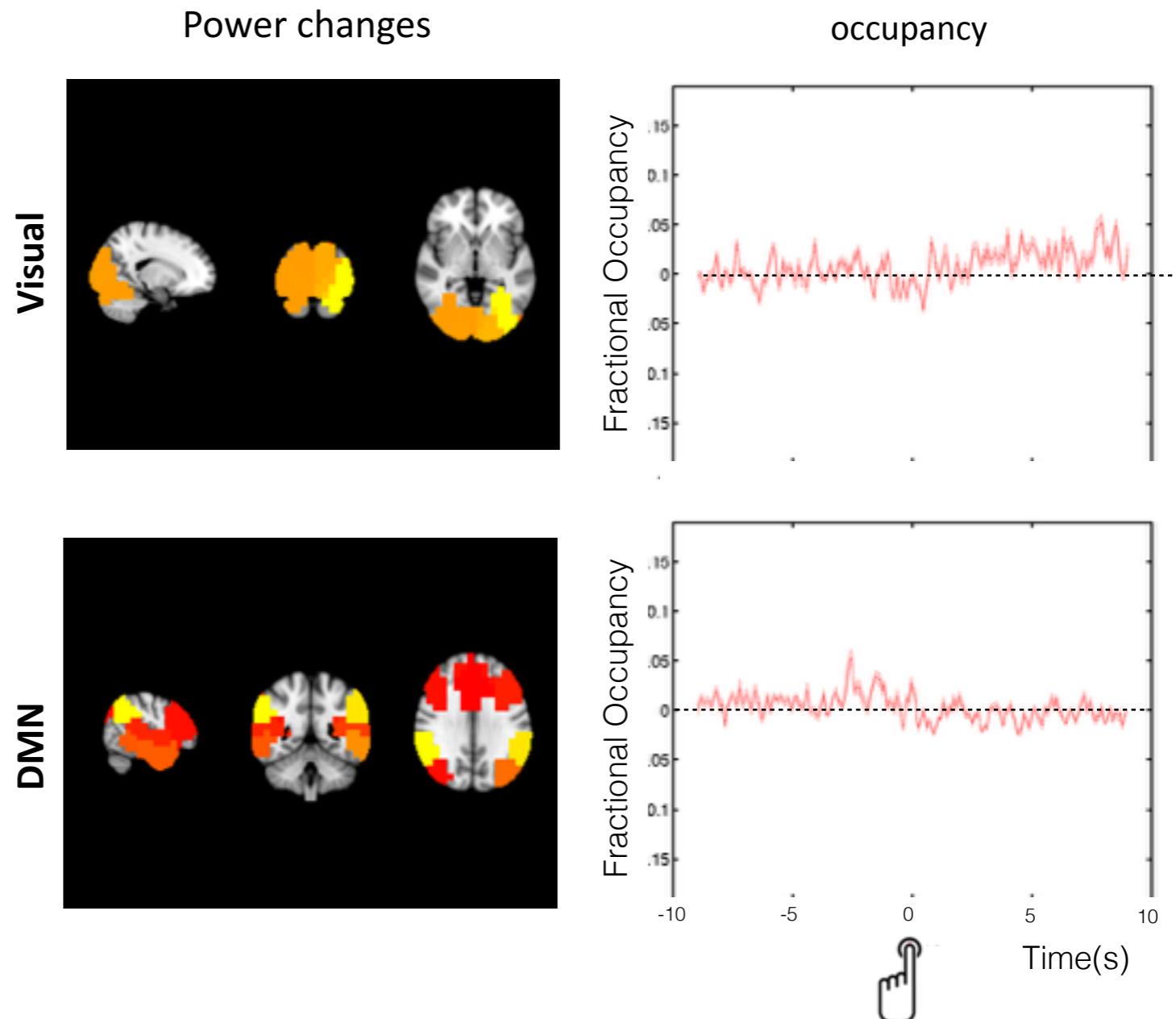
HMM-Gaussian

- Task-related HMM states
 - 10 subjects
 - 4-30Hz
 - 8 HMM states



HMM-Gaussian

- **Task-unrelated HMM states**
 - 10 subjects
 - 4-30Hz
 - 8 HMM states



HMM-Gaussian

To set an HMM-Gaussian:

```
> options = struct();
> options.K = 8;
> options.order = 0;
> options.zeromean = 0;
> options.covtype='full';
> [hmm,Gamma] = hmmpar(X,T,options);
```

No. of states

Model the mean

Full connectivity

HMM structure

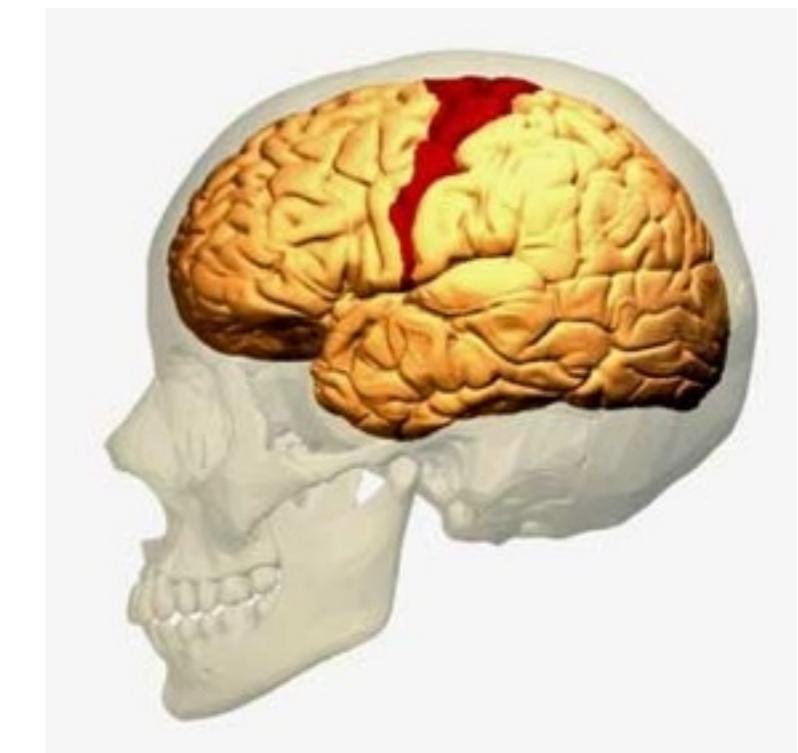
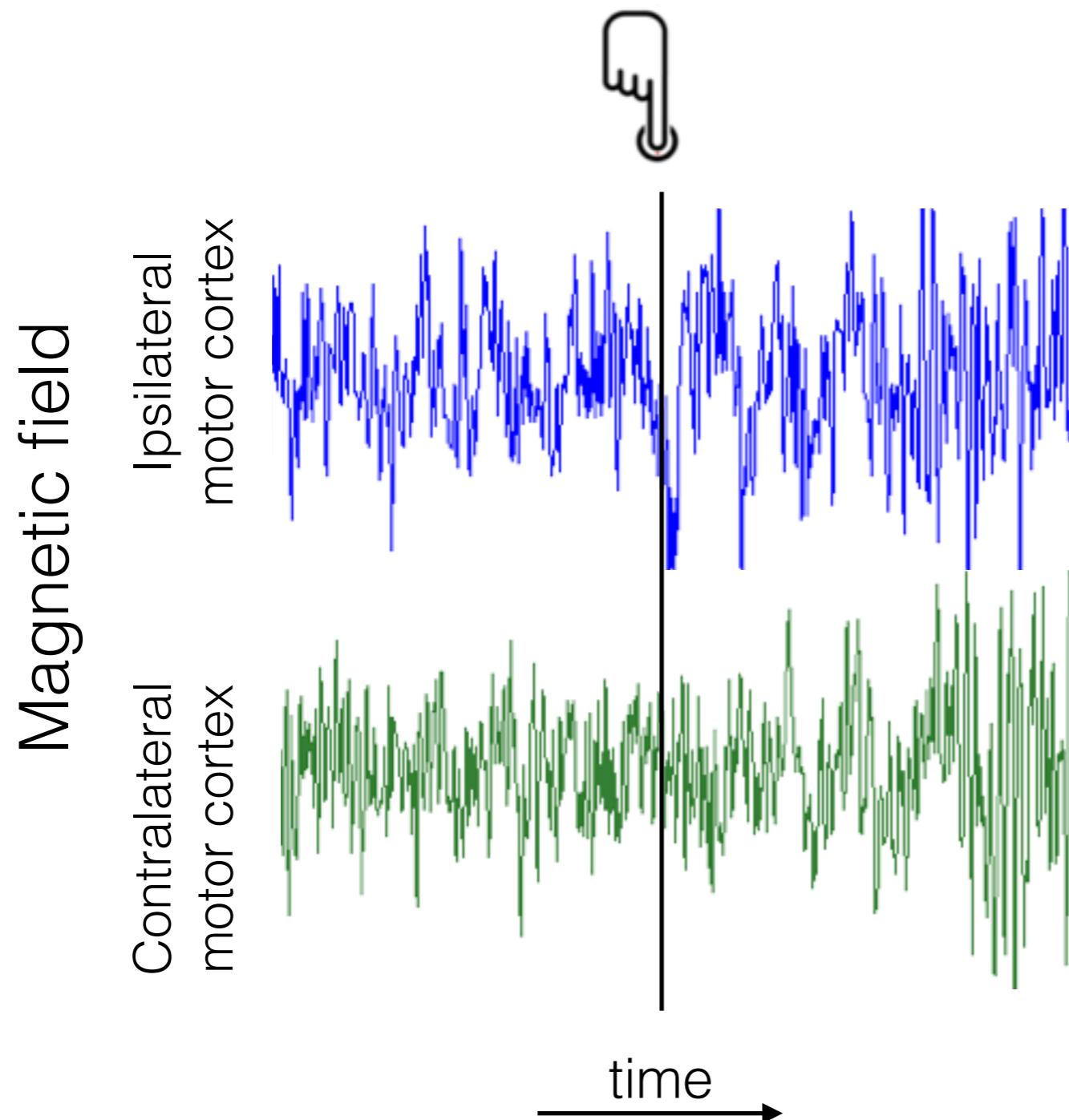
State time courses

HMM-Gaussian

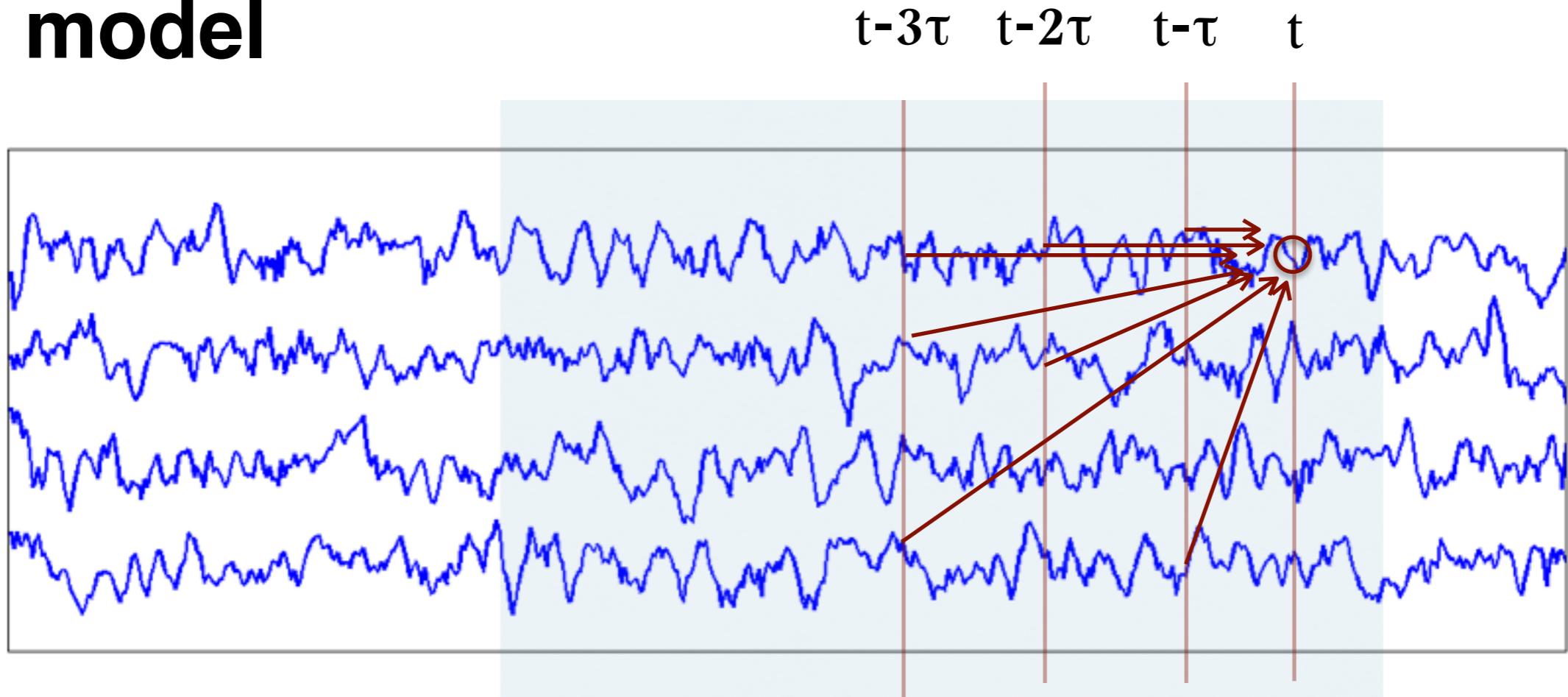
In summary:

- The *HMM-Gaussian* focuses on **power** and **can be applied to whole brain**
- But: is insensitive to phase and is not frequency-resolved

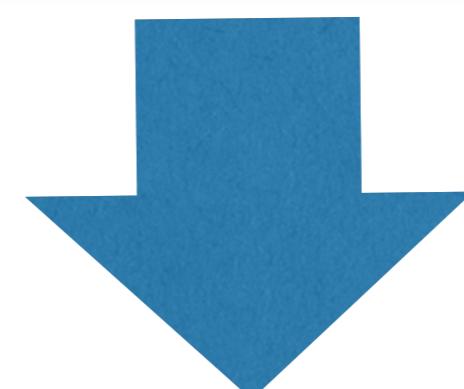
what about working with raw time courses?
e.g. can we then find time-varying phase locking?



MAR model



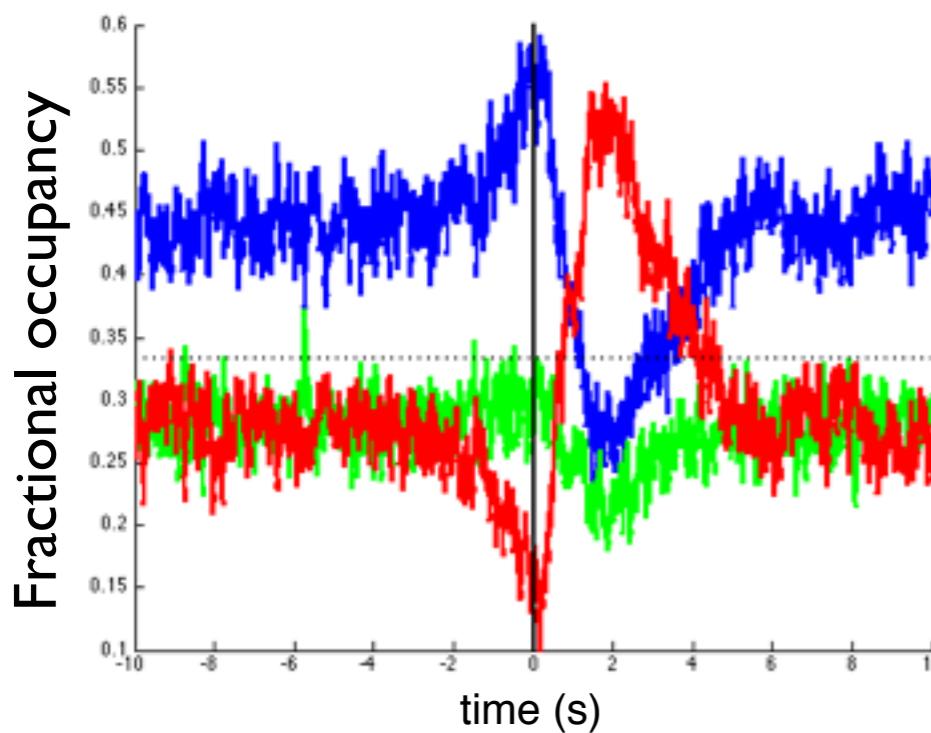
Contains

- 
- Power spectral density
 - Coherence
 - Directed coherence
 - Phase

MAR model

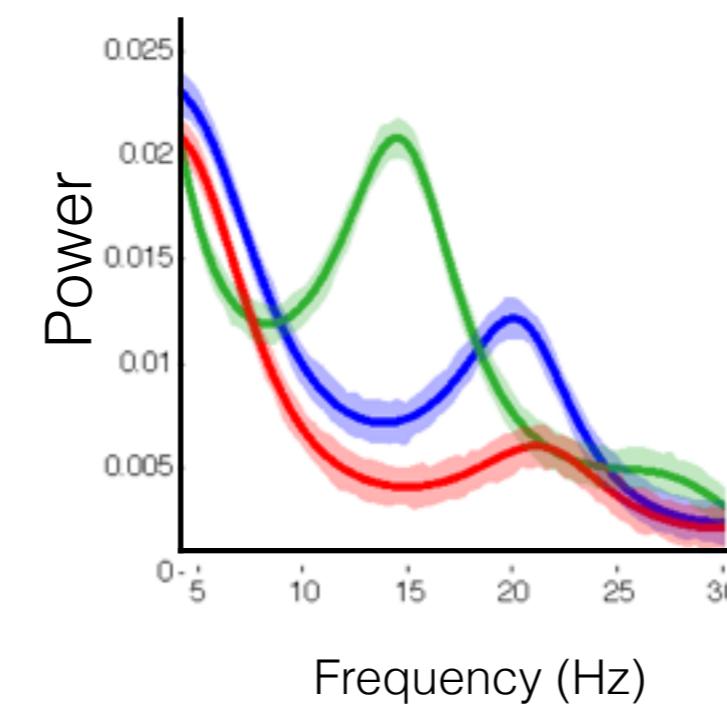
- The MAR contains information about **phase**
- It is **spectrally resolved**, i.e. all of these quantities (power, coherence, phase relations) are defined as a function of frequency

HMM state time-courses

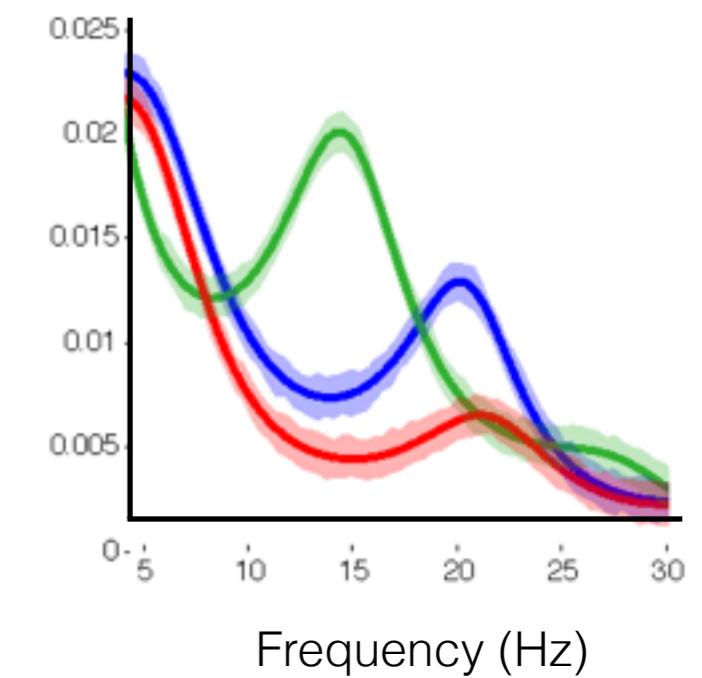


Finger-tap (beta suppression)
Post-finger-tap (beta rebound)
Baseline

Spectral properties of each HMM state

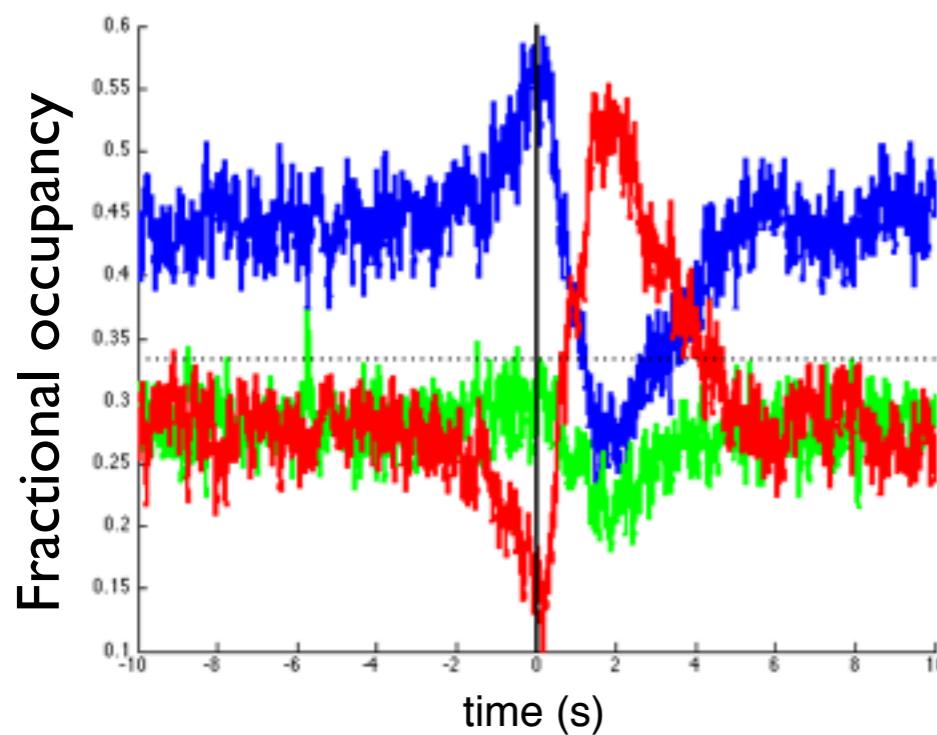


- significant state-dependent (time-varying) power spectra



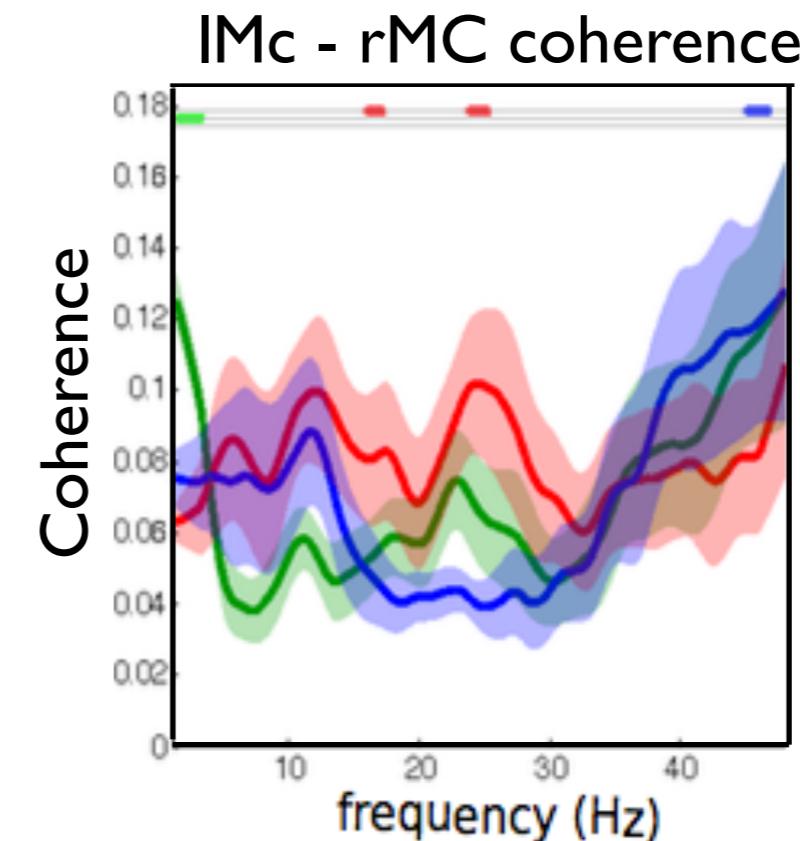
HMM-MAR

HMM state time-courses



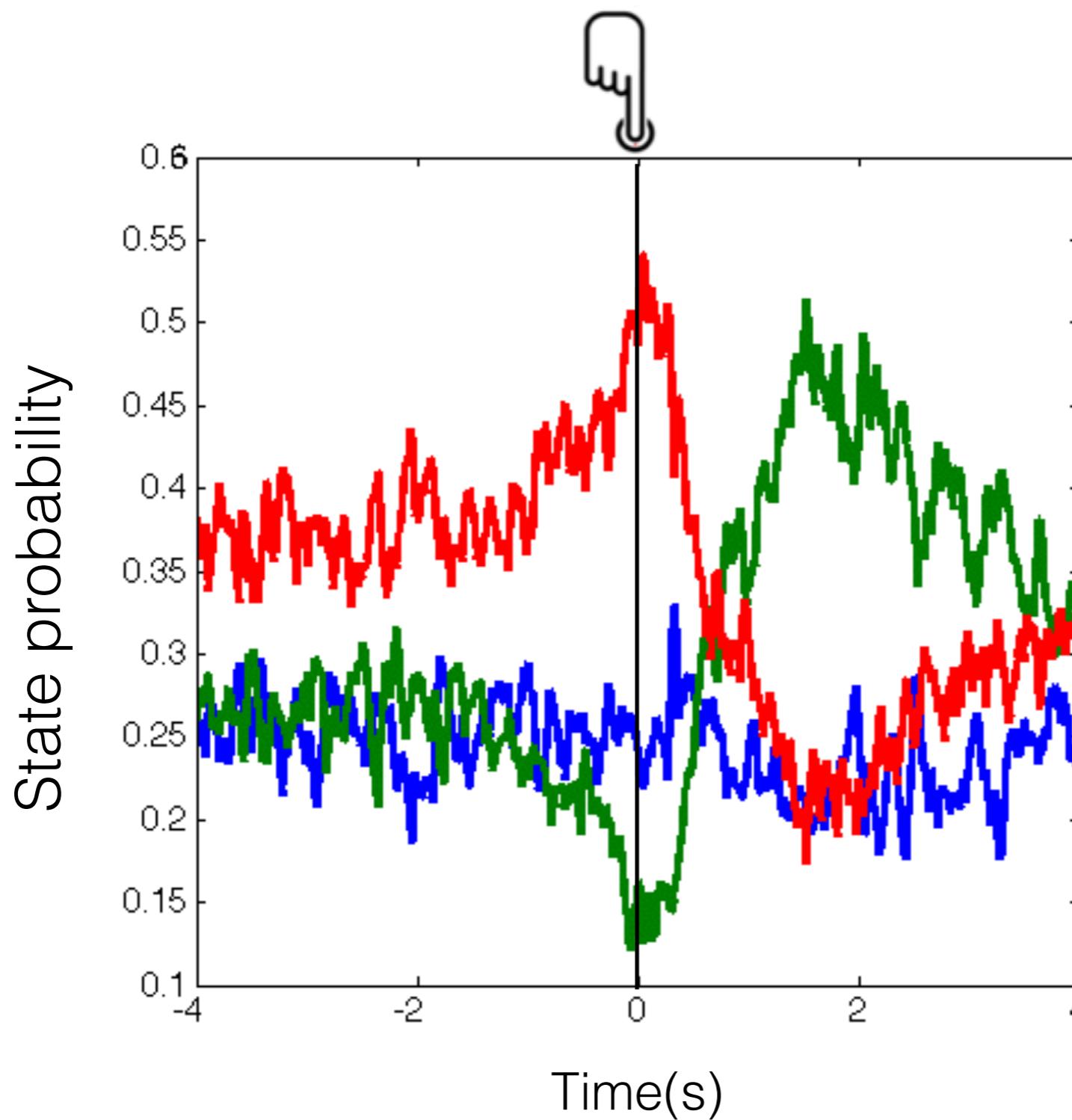
Finger-tap (beta suppression)
Post-finger-tap (beta rebound)
Baseline

Cross-Spectral properties of each HMM state

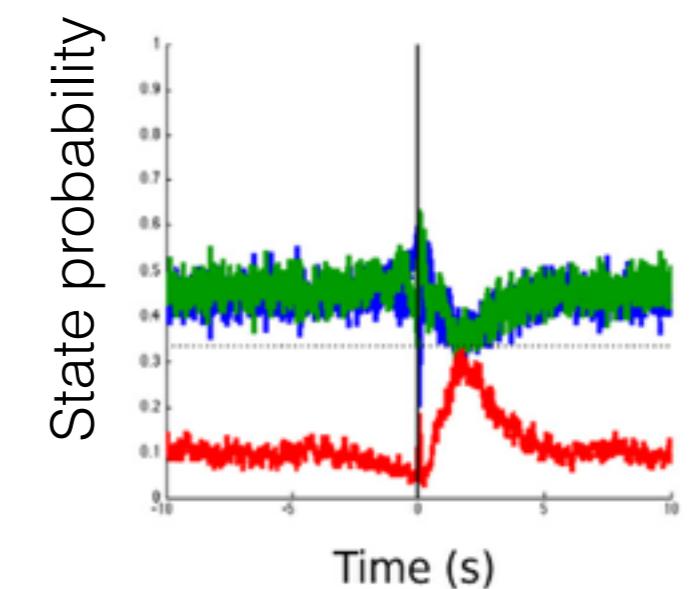


- significant state dependent (time-varying) coherence (phase locking)

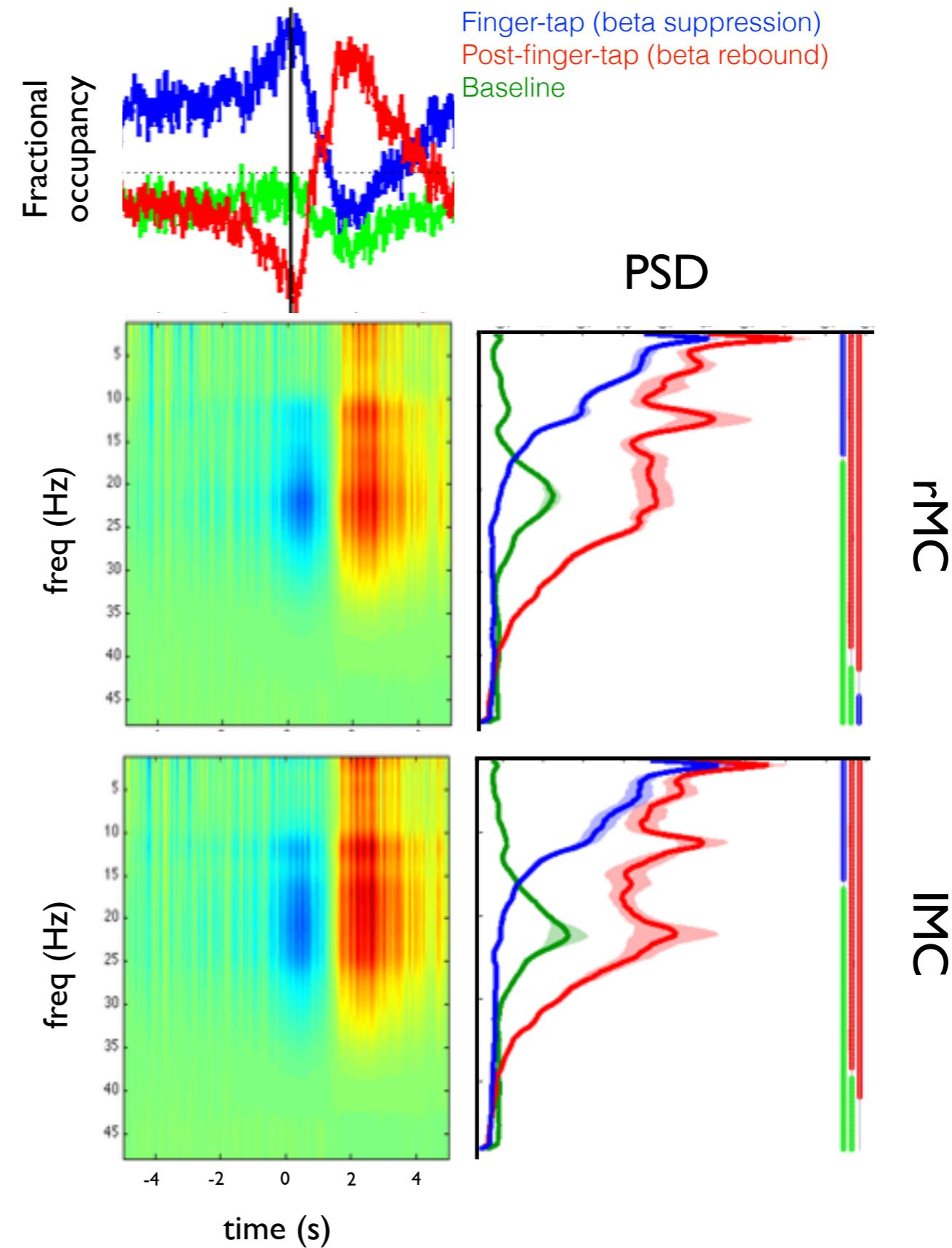
HMM-MAR



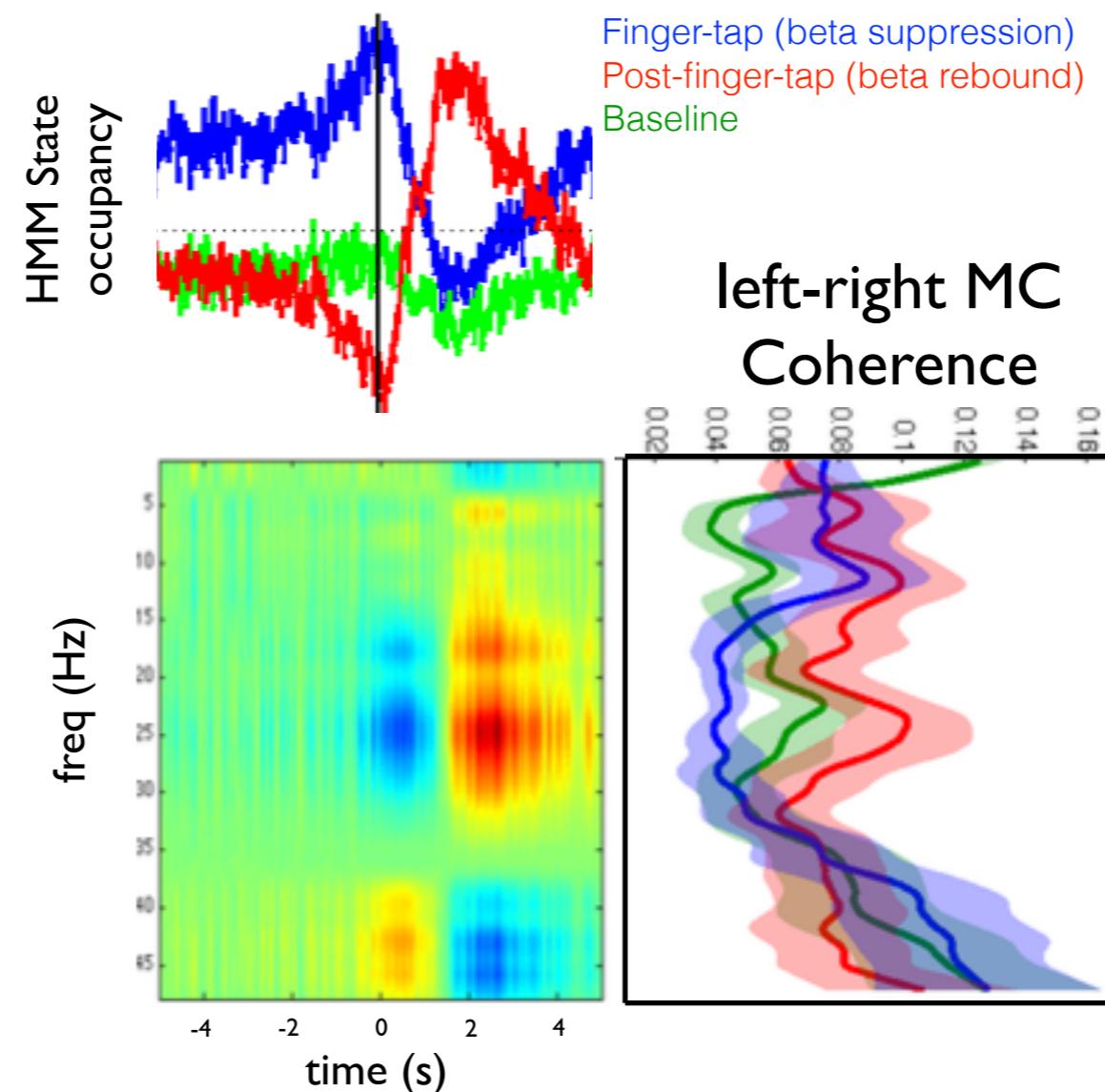
HMM-Gaussian



Computing T-F Maps from HMM

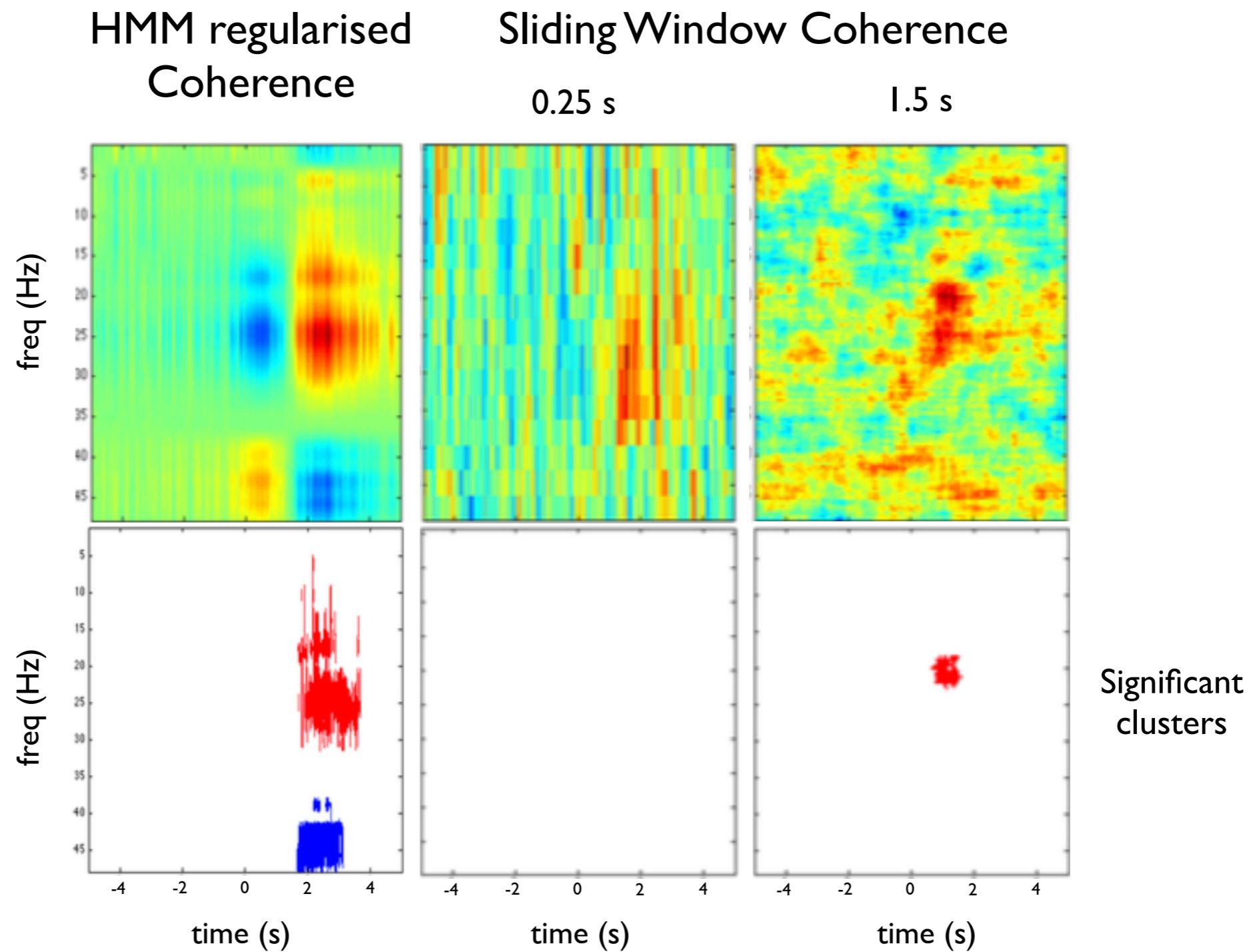


HMM-MAR



HMM regularise
Coherence

HMM-MAR



To set an HMM-MAR:

```
> options = struct();
> options.K = 3;
> options.order = 5;
> options.zeromean = 1;
> options.covtype='diag';
> [hmm,Gamma] = hmmdmar(X,T,options);
```

No. of states

MAR order

HMM structure

State time courses

Hidden Markov Model

In summary:

- The *HMM-Gaussian* approach focuses on power and **can be applied to whole brain**
- The *HMM-MAR* works on the raw time series and **is sensitive to phase information**, and is applicable to low-to-medium number of regions

More info in : <https://github.com/OHBA-analysis/HMM-MAR/wiki>

Hidden Markov Model

In the practicals

1. We will apply the *HMM-Gaussian* on resting state whole brain MEG data and find resting state networks that are defined in terms of activation and functional connectivity (power correlation)

2. We will apply the *HMM-MAR* on two motor regions to capture quick changes elicited during a motor task, in terms of power changes and phase coupling