

# Team MedX Hackers – Technical & Application Report

## Literature Review

Electrocardiogram (ECG) based arrhythmia classification has been extensively studied due to its critical role in the early diagnosis and management of cardiovascular diseases. Traditional ECG interpretation relies heavily on expert analysis, which is time-consuming and prone to inter-observer variability. Consequently, automated arrhythmia detection methods have gained significant attention, particularly with the availability of publicly accessible ECG datasets and advances in deep learning.

One of the major drivers of recent progress in ECG analysis is the release of large-scale, annotated datasets. The PTB-XL dataset provides a comprehensive collection of clinically labeled ECG recordings covering a wide range of diagnostic classes [1]. Although PTB-XL is widely used for recording-level diagnosis, many arrhythmia studies continue to rely on the MIT-BIH Arrhythmia Database due to its detailed beat-level annotations and suitability for heartbeat classification tasks.

A systematic benchmarking study of deep learning models for ECG analysis was conducted and demonstrated that convolutional neural networks (CNN) based and CNN derived architectures achieve strong classification performance [2]. Their results highlight the ability of deep models to capture morphological and temporal characteristics of ECG signals, while also identifying challenges related to generalization across patient populations and class imbalance.

Several studies have specifically focused on CNN based heartbeat and arrhythmia classification using datasets such as MIT-BIH. A deep learning framework was introduced later for ECG heartbeat classification and showed that end-to-end CNN models outperform traditional machine-learning approaches based on handcrafted features [3]. Those findings indicate that automatic feature extraction using convolutional architectures improves classification accuracy while simplifying the overall processing pipeline.

In addition to performance-oriented studies, recent survey papers have analyzed broader challenges in automated arrhythmia detection. Such identified key issues from a recent study included signal noise, data imbalance, and limited interpretability of deep models [4]. The review emphasizes the importance of robust preprocessing, balanced training strategies, and model transparency for reliable deployment in clinical environments. Despite these advances, existing work often prioritizes either high classification accuracy or large-scale benchmarking, with limited emphasis on computational efficiency and deployment feasibility. Motivated by these gaps, the proposed work employs a compact one-dimensional CNN architecture evaluated using the MIT-BIH Arrhythmia Database. The focus on lightweight model design, clearly defined preprocessing, and systematic validation aims to achieve reliable arrhythmia classification suitable for practical healthcare applications such as real-time monitoring and clinical decision support.

## Problem Identification

**The Challenge of Global Health:** The challenge posed by cardiovascular diseases (CVDs) are considered the first cause of mortality in all countries and represents a considerable proportion of global deaths annually. Arrhythmias (abnormal cardiac rhythm patterns that can be the first signs of fatal conditions such as stroke, myocardial infarction, and sudden cardiac arrest) are some of the most important signs of cardiac health. Continuous monitoring is a necessity for millions of patients around the world if these abnormalities are to be detected before they turn into life-threatening situations.

**Clinical Bottleneck:** The manual interpretation of Electrocardiogram (ECG) data by qualified cardiologists is a major component of the current standard for diagnosing arrhythmias. Although this approach works well for

short-term assessments, it becomes ineffective for long-term monitoring (e.g., using Holter monitors), where a single patient may produce more than 100,000 heartbeats in a 24-hour period. Examining such enormous volumes of data is:

- **Time-consuming:** Diagnosis and treatment are severely delayed.
- **Error-prone:** Misinterpretation or missed diagnosis may result from clinician weariness and the subtlety of some signal fluctuations.
- **Subjective:** Different experts may interpret things differently.

**The Unfulfilled Need:** An automated, dependable, real-time diagnostic solution that can immediately process raw ECG signals is desperately needed. Additionally, many patients do not have timely access to professional interpretation due to the acute dearth of cardiologists in underserved and rural areas. By using an AI-driven approach to automate the classification of arrhythmia types, our project fills these gaps and guarantees quick, precise, and accessible cardiac diagnostics regardless of location.

## Dataset Justification

**Source and Content:** We made use of the MIT-BIH Arrhythmia Database, which is accessible through the open-source Kaggle repository (which was initially curated by PhysioNet). For studies on arrhythmia analysis, this dataset is commonly regarded as the gold standard. It is made up of 48 half-hour segments of two-channel ambulatory ECG recordings from 47 participants that the BIH Arrhythmia Laboratory examined.

### Dataset Statistics:

- **Total Records:** Approximately 109,000 segmented heartbeat samples (about 87,000 for training and 21,000 for testing).
- **Features:** Each sample is a 360 Hz segmented ECG heartbeat signal (time-series).
- **Labels:** Five heartbeat classes (AAMI standard):
  - N: Normal beat
  - S: Supraventricular premature beat
  - V: Premature ventricular contraction
  - F: Fusion of ventricular and normal beat
  - Q: Unclassifiable beat

**Rationale for the Choice:** Three main factors led us to choose this dataset:

- **Clinical Relevance:** Captures real-world physiological noise and variability.
- **Volume for Deep Learning:** Sufficient sample size to train model without overfitting.
- **Benchmarking:** Common reference dataset enables direct comparison with prior work.

## Methodology

**Data Preprocessing:** The ECG data were taken from the MIT-BIH arrhythmia dataset with each ECG containing 187 values of time-domain signals that represent a single heartbeat and the last column representing the

class of arrhythmia. The dataset was imbalanced when it came to classes, so downsampling and upsampling were used together to create a balanced distribution of all five classes. StandardScaler was applied in order to standardize the signal values and help with convergence of the model. Reshaping of data was done to turn into a 3D data structure to be used as input for 1D convolutional neural networks. To create more robust models and to improve generalization of the models, techniques of augmentation through adding Gaussian noise, shifting in time, and adjusting amplitude were applied to the data

**Model Architecture:** Hybridization of CNNs and BiLSTMs to classify ECG data developed in this study. CNNs (convolutional neural networks) were utilized to extract localized morphology features (i.e., QRS waves), with batch normalization, max pooling and dropout utilized to reduce overfitting of CNN features. Bidirectional LSTM (long short term memory) networks were employed to capture temporal dependencies among ECG signals. Global average pooling followed by Fully Connected networks (FC) provided a softmax layer to produce probabilities for each arrhythmia class identified in this task.

**Training and Validation Strategy:** The Adam optimiser and a categorical cross-entropy loss function were used to train the model. A balanced dataset was stratified and split into 85% training and 15% validation for use in training and validating a custom training loop. Finally, we utilised a custom training approach that included early stopping and a learning rate reduction to reduce overfitting. Finally, we evaluated the model on an unseen test dataset for performance evaluation after training was complete.

## Pretrained Model Usage & Adaptation

This study developed a tailored, from-scratch CNN-BiLSTM architecture to address the specific requirements of ECG time-series data rather than relying on an external pretrained model. External pretrained models used for images or text were eliminated because they were not applicable to physiological signals due to the difference in their physical domains and the limited amount of transferable information that can be learned from one domain to another. Some potential risks associated with this study include dataset bias ness (i.e., bias introduced by having too few examples), poor variations in quality of ECG signals, and poorer generalization ability to disparate populations or devices as compared to a more generalized population/device model. The proposed system can be utilized in real-time cardiovascular monitoring platforms that incorporate either wearable ECG devices or clinical monitoring systems. It facilitates automated detection of arrhythmias, creation of early warning alerts for clinicians, and provides clinical decision support to physicians. Nevertheless, medical monitoring is still required for these products, in order to ensure their safe and dependable usage.

## Results

### Learning Curves

Figure 1 shows accuracy and loss trends over epochs. Both training and validation accuracy increase rapidly and stabilize in the high-0.97 range. Training and validation loss decrease smoothly and converge, with no significant divergence between curves, suggesting stable training and limited overfitting.

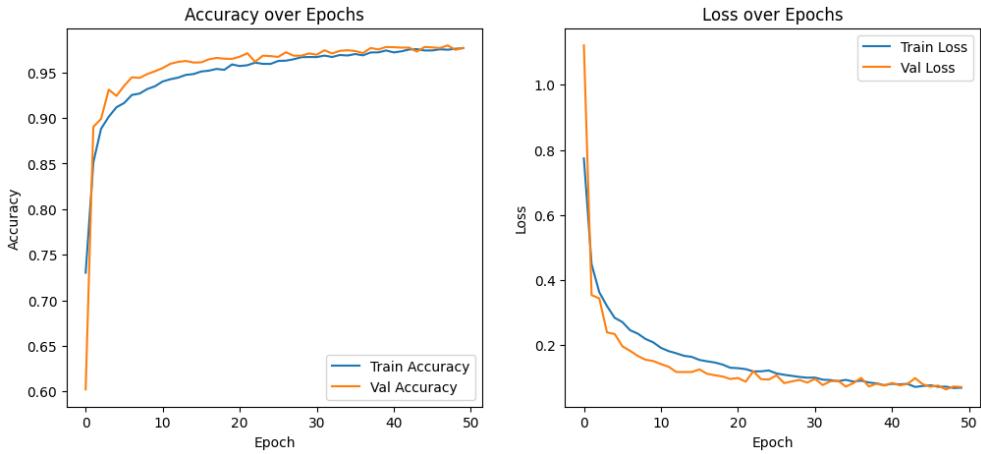


Figure 1: Training dynamics: accuracy and loss over epochs.

## Confusion Matrices and Error Patterns

Figure 2 summarizes the validation and unseen test confusion matrices. Most predictions lie on the diagonal, indicating strong class-wise recognition. Remaining errors concentrate in clinically similar or minority classes and are affected by class imbalance. The *Normal* class dominates, and a small fraction of S/F/V samples are occasionally misclassified as Normal or confused among each other. Overall, the model generalizes well to unseen data and maintains consistent behavior across validation and test distributions.

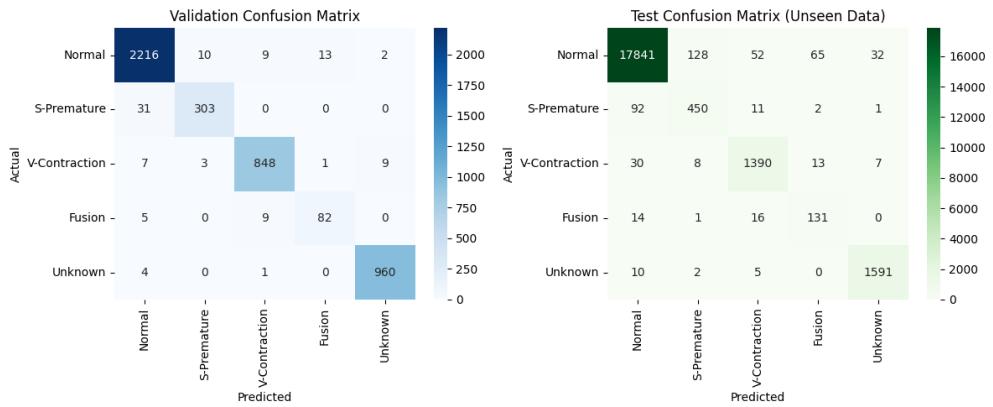


Figure 2: Confusion matrices on validation data and unseen test data.

## Limitations

- MIT-BIH demographic and device diversity is limited. So external validation is needed.
- Beat-level classification does not directly capture multi-beat rhythm context in complex arrhythmia situations.

## Real-World Applications

This ECG arrhythmia classification system integrates with real-time cardiac monitoring platforms including wearables, Holter monitors, and hospital systems, enabling consistent and rapid ECG analysis for quick arrhythmia identification. The system reduces manual workload for cardiologists, supports efficient resource allocation to high-risk patients, and enhances telemedicine and remote monitoring services. It functions as a

clinical decision-support tool that improves patient safety through accurate classification rather than replacing physician judgment.

## Marketing & Impact Strategy

**Target Market & Adoption:** This ECG classification system targets hospitals, cardiac centers, telemedicine platforms, and rural clinics with limited cardiologist access. Implementation follows three stages: pilot testing at teaching hospitals, integration with hospital IT systems, and expansion to remote patient monitoring.

**Clinical Benefits & Cost Savings:** The automated system reduces ECG interpretation time from 15 minutes to 2 seconds while cutting costs from \$50-150 to approximately \$5 per analysis. A mid-sized facility processing 200 ECGs daily could save over \$1.5 million annually, and faster arrhythmia detection enables earlier intervention to reduce stroke risk and prevent sudden cardiac events.

**Market Access Strategy & Social Impact:** Building clinical trust requires live demonstrations at major cardiology conferences and validation studies published in journals like Circulation and JACC. Partnerships with ECG manufacturers enable bundled solutions that simplify hospital procurement, while mobile-optimized design with offline capabilities allows rural clinics to perform advanced diagnostics without on-site specialists.

## Future Improvements

**Architecture Enhancement:** The current model analyzes single-lead ECG recordings, but expanding to 12-lead analysis would capture comprehensive cardiac data and detect region-specific abnormalities. Integrating attention mechanisms based on Transformer architecture would highlight which waveform features influenced each diagnosis, making results more interpretable and trustworthy for clinicians.

**Dataset Diversification:** While MIT-BIH provides solid training data with over 100,000 samples, it has demographic limitations. Future work should incorporate other large datasets to better represent diverse patient populations and various ECG equipment types. Including more pediatric and elderly patient recordings would also make the system useful across all age ranges.

**Deployment Optimization & Regulatory Compliance:** Model compression reduces size by 70-80% for smartwatch deployment while maintaining accuracy and enabling 500+ Hz real-time processing. Clinical deployment requires validation studies against cardiologists for FDA 510(k) and CE marking, plus HIPAA-compliant infrastructure with encryption.

## References

- [1] P. Wagner *et al.*, “PTB-XL, a large publicly available electrocardiography dataset,” *Scientific Data*, vol. 7, no. 1, pp. 1–15, 2020.
- [2] N. Strothoff *et al.*, “Deep learning for ECG analysis: Benchmarks and insights from PTB-XL,” *IEEE Journal of Biomedical and Health Informatics*, vol. 25, no. 5, pp. 1519–1528, 2020.
- [3] G. Sannino and G. De Pietro, “A deep learning approach for ECG-based heartbeat classification for arrhythmia detection,” *Future Generation Computer Systems*, vol. 86, pp. 446–455, 2018.
- [4] G. Swapna, K. P. Soman, and R. Vinayakumar, “Automated detection of cardiac arrhythmia using deep learning techniques,” *Procedia Computer Science*, vol. 132, pp. 1192–1201, 2018.