

Fundamentals of X-ray Computed Tomography

Tomography: chụp cắt lớp



Part I : the very very basics

Part II : components and physics

Part III : recent advances in CT

Part IV : some images

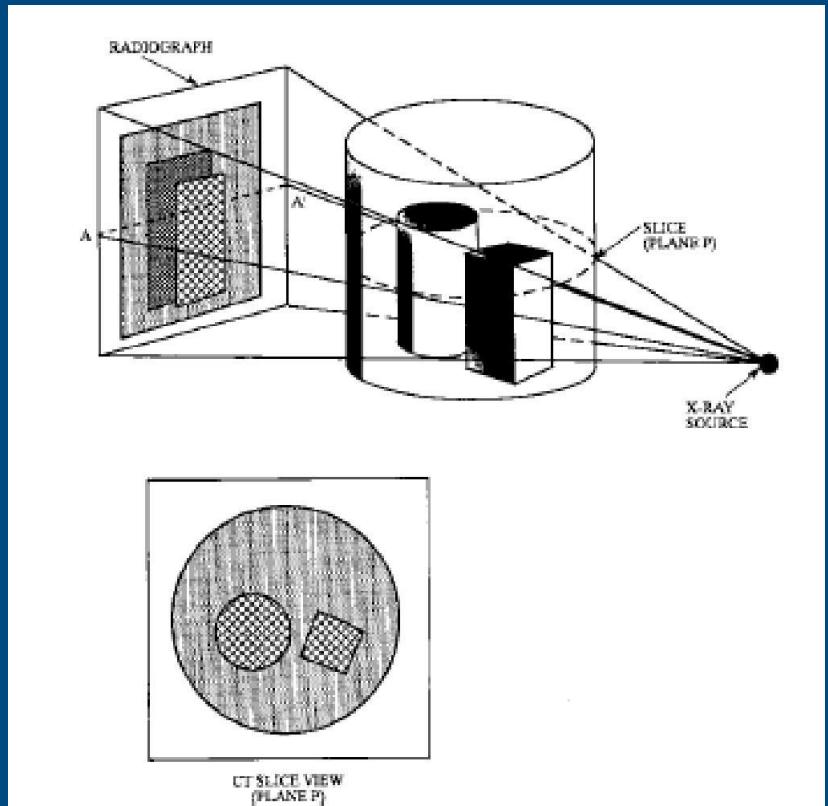
CT: Computed Tomography

CAT: Computerized Axial Tomography

CAT: Computer Assisted Tomography

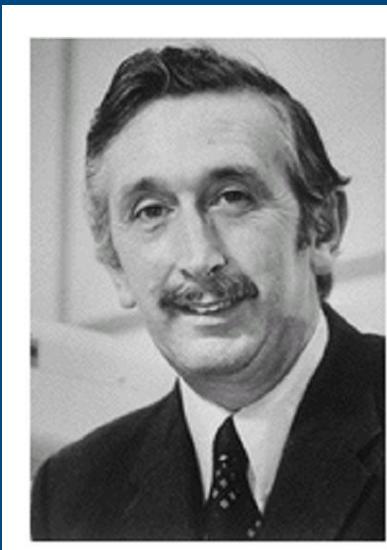
- Pass x-rays through patient
- Detect on the other side
- Repeat from all angles surrounding patient
- Reconstruct cross sectional images
- Pixel values represent attenuation of tissue

tomography <τοπος – γραφειν>

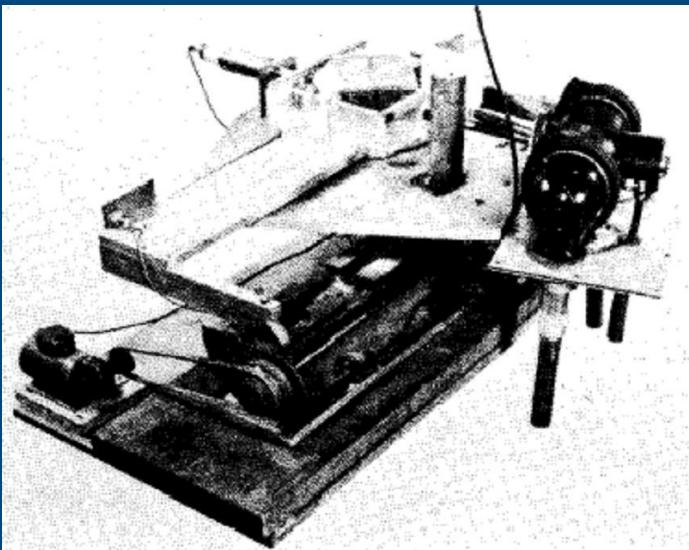


Sir Godfrey N. Hounsfield (1971)

G. N. Hounsfield



Laboratory CT device



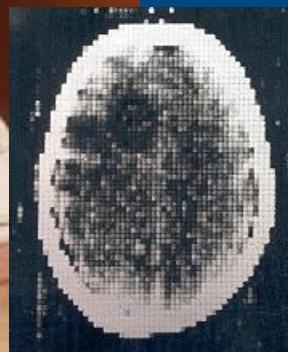
Brain image



<http://www.nobel.se/medicine/laureates/1979/hounsfield-lecture.pdf>

Over 30 years of advances in CT

1972 - EMI Scanner



2002 - Lightspeed 16



5 min

Scan time/image

0.5 sec

80x80

Image size

512x512

3 lp/cm

Spatial resolution

15 lp/cm

5mm/5HU/50 mGy

Contrast resolution

3mm/3HU/30 mGy

A few

Slices to review

100 - 1000

I Can See Clearly Now
(Johnny Nash)

Hit song

Can't Get You Out Of My Head
(Kylie Minogue)

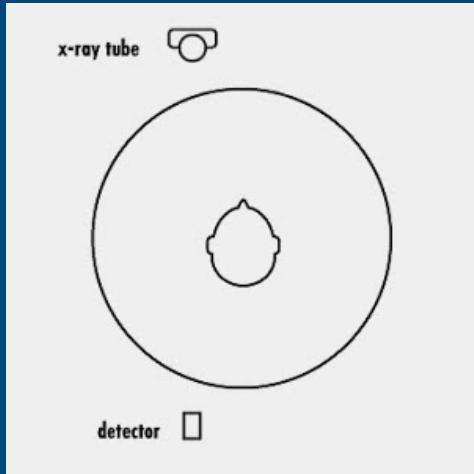
2014: CT Revolution

Introduction

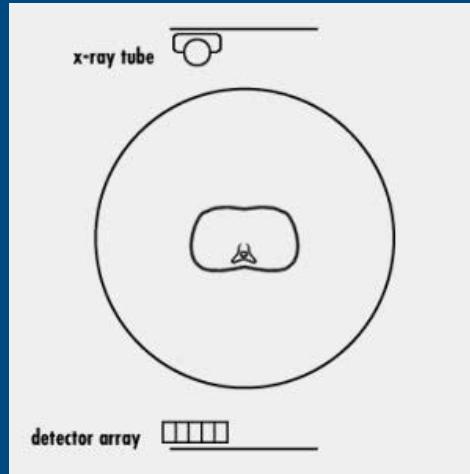
Cardiac application

CT scanner generations

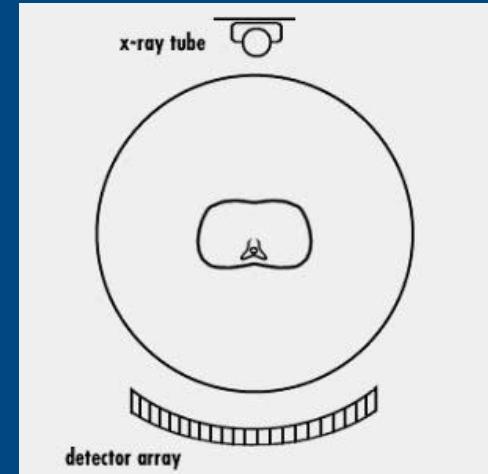
1st generation



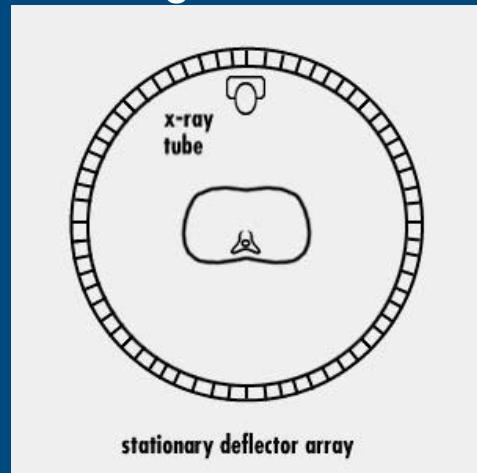
2nd generation



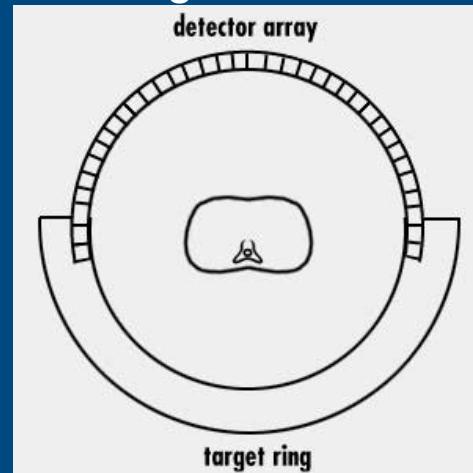
3rd generation



4th generation



5th generation

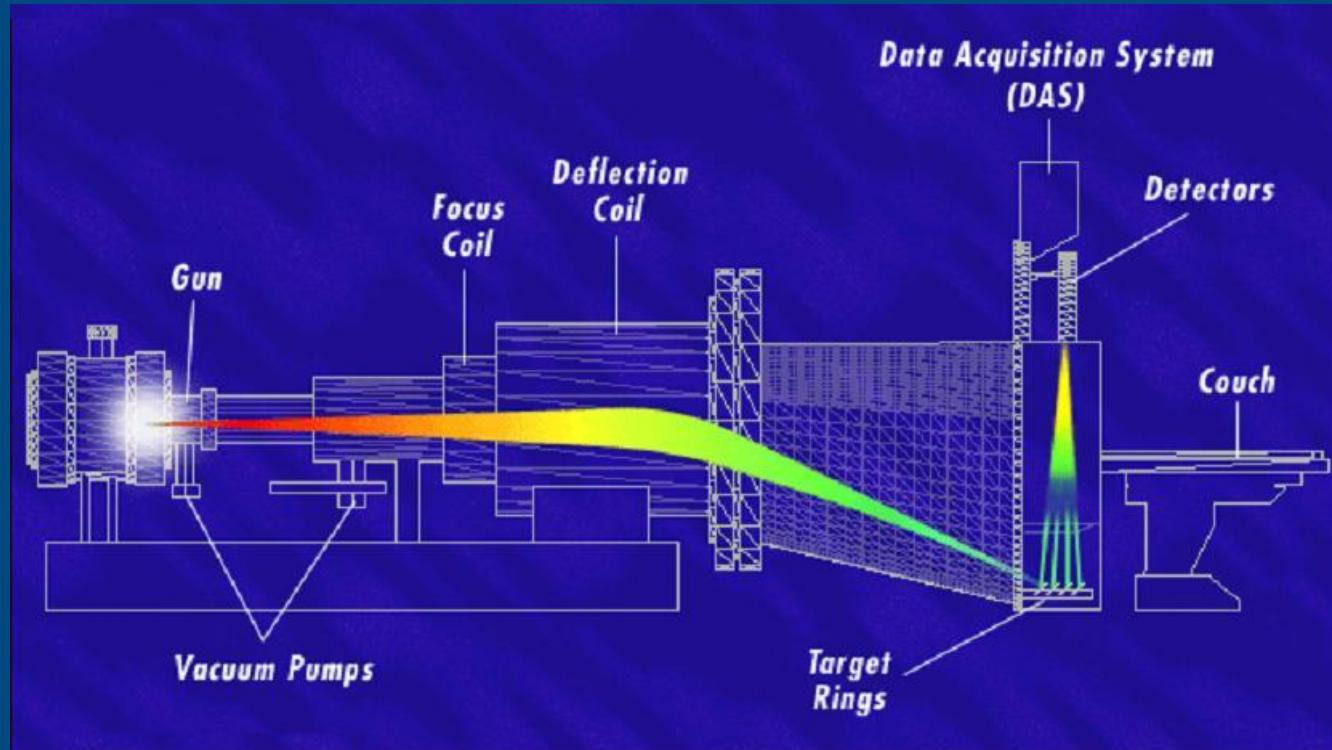
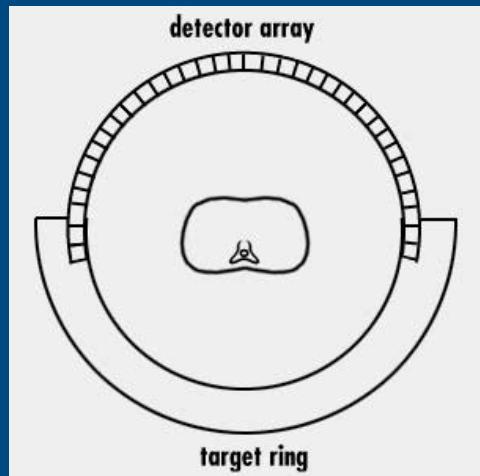


7 Hiện tại tất cả đang dùng 3rd generation
4th generation và 5th rất là đắt

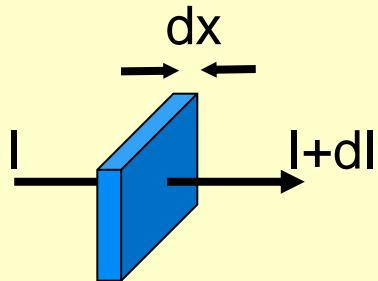
Courtesy of Bruno De Man, GE Global Research
< Courtesy of ??? >

Electron beam tomography / e-Speed

5th generation

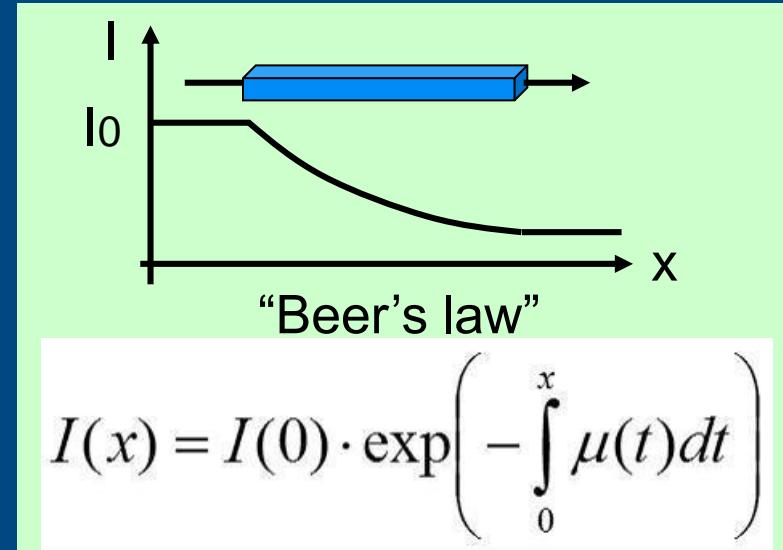


Beer's law

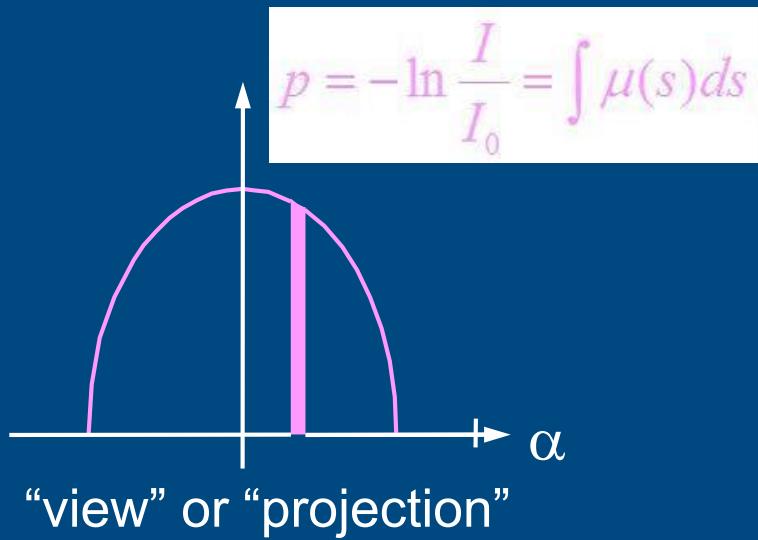
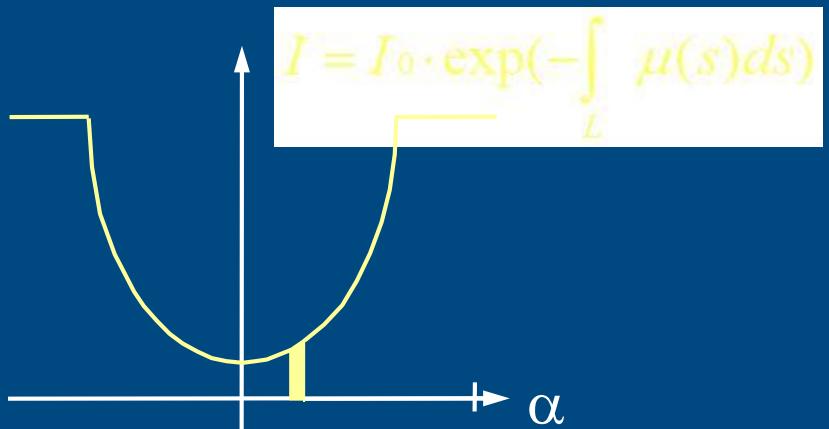
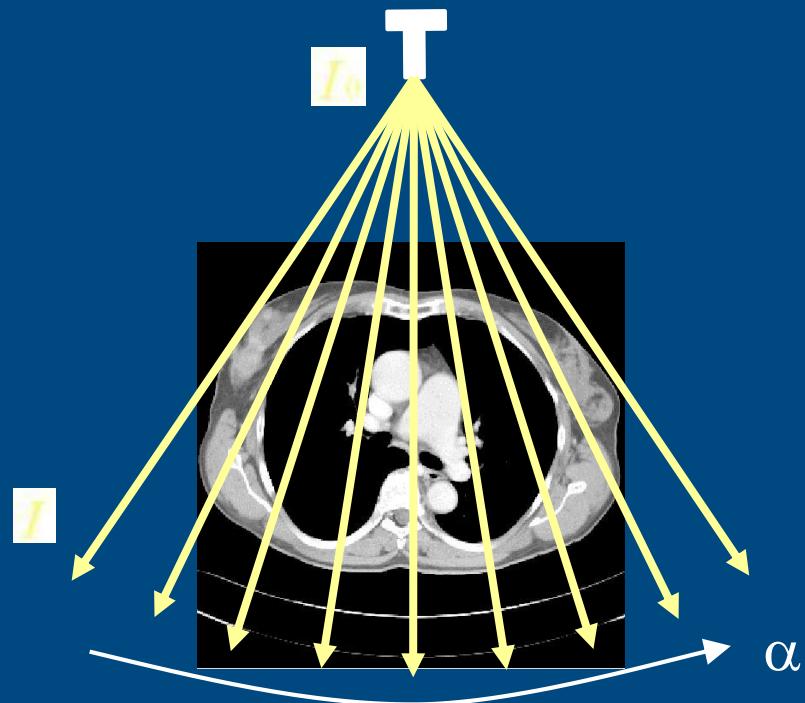


“Linear attenuation coefficient”

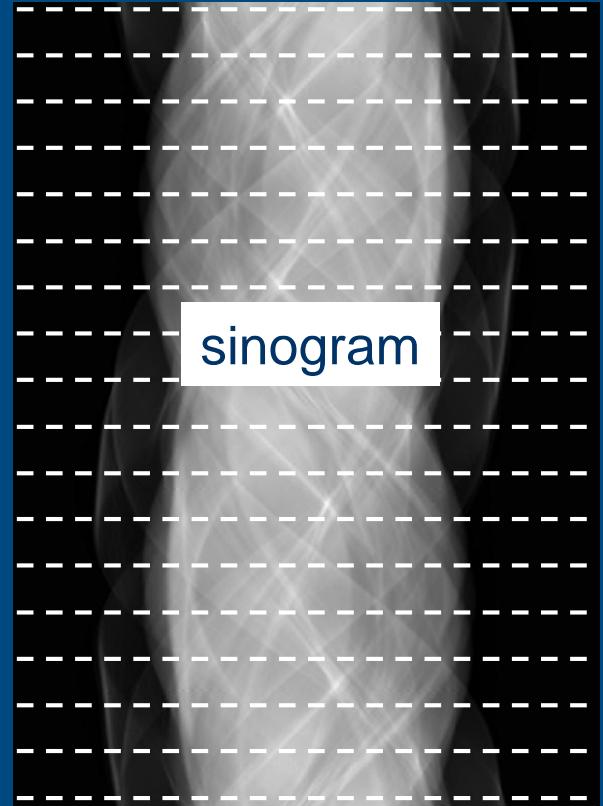
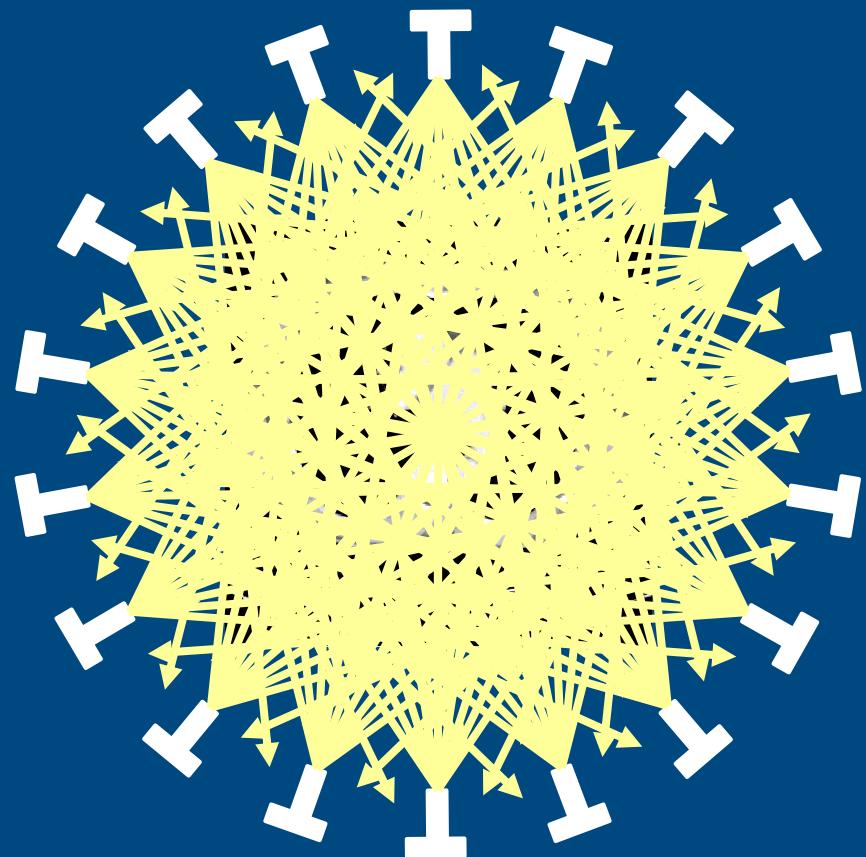
$$\mu = -\frac{\partial I / \partial x}{I}$$



Measuring attenuation line integrals



Sinogram



11

nombre de ligne est le nombre des images
nombre de colonne est le nombre de pixel

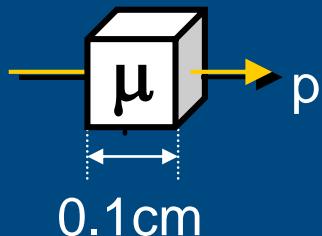
Courtesy of Bruno De Man, GE Global Research

mu comme la densité/surface

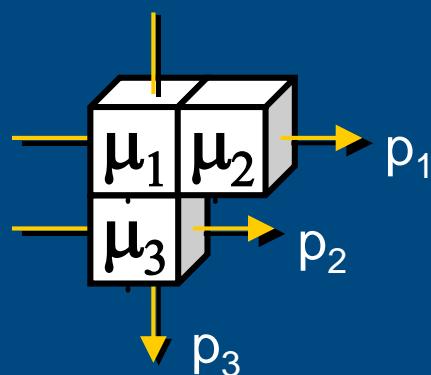
imagination at work



Image reconstruction

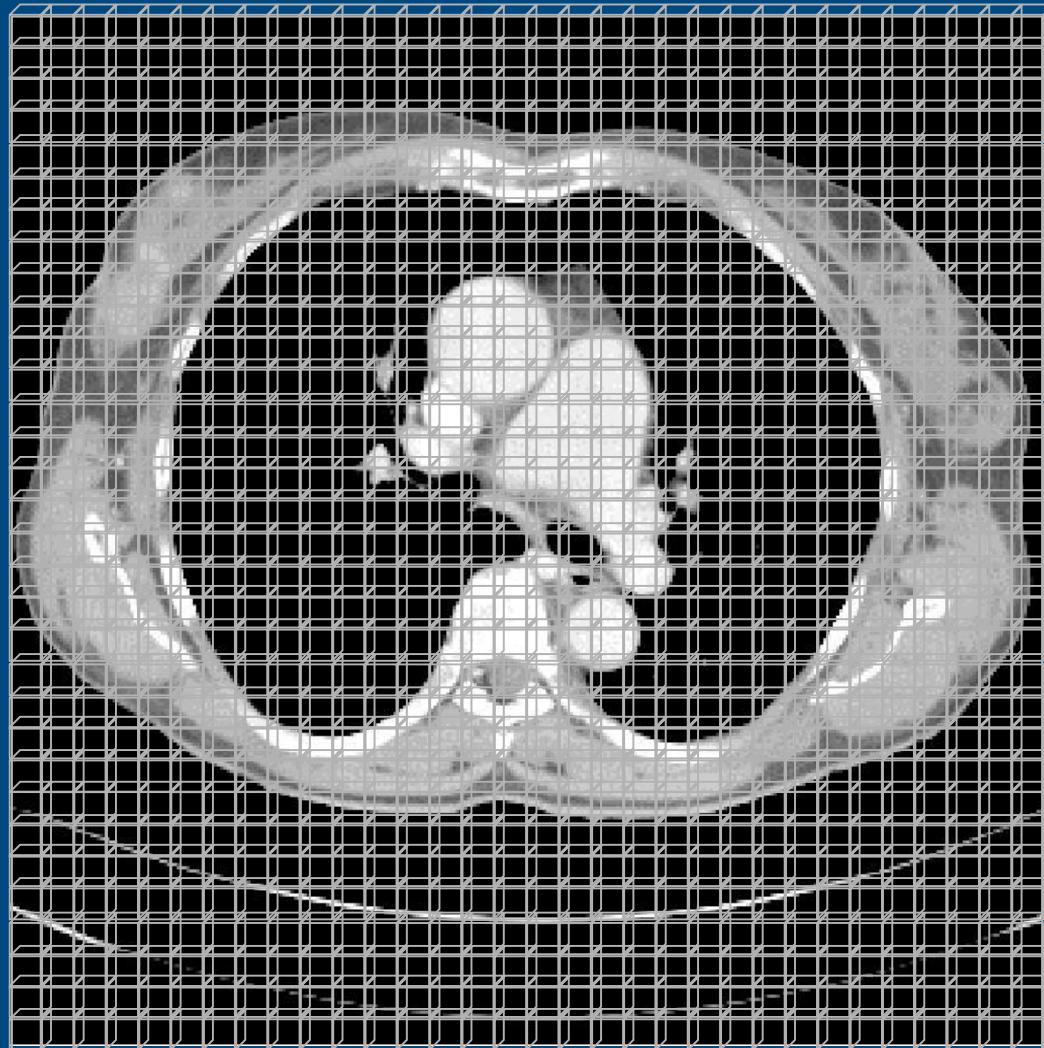


$$p = 0.02 \rightarrow \mu_1 \cdot 0.1\text{cm} = 0.02 \rightarrow \mu_1 = 0.2\text{cm}^{-1}$$



$$\begin{aligned} p_1 &= 0.06 & (\mu_1 + \mu_2) \cdot 0.1\text{cm} &= 0.06 \\ p_2 &= 0.01 & \mu_3 \cdot 0.1\text{cm} &= 0.01 \\ p_3 &= 0.03 & (\mu_1 + \mu_3) \cdot 0.1\text{cm} &= 0.03 \end{aligned} \rightarrow \begin{aligned} \mu_1 &= 0.2\text{cm}^{-1} \\ \mu_2 &= 0.4\text{cm}^{-1} \\ \mu_3 &= 0.1\text{cm}^{-1} \end{aligned}$$

Image reconstruction



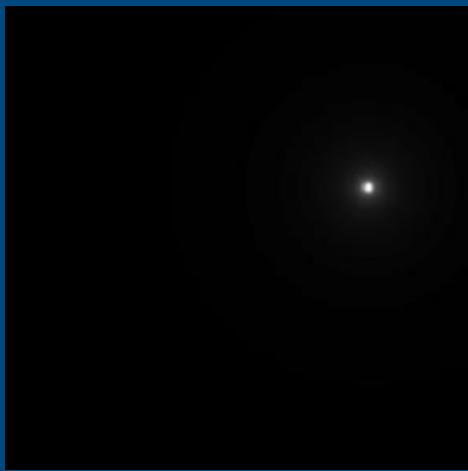
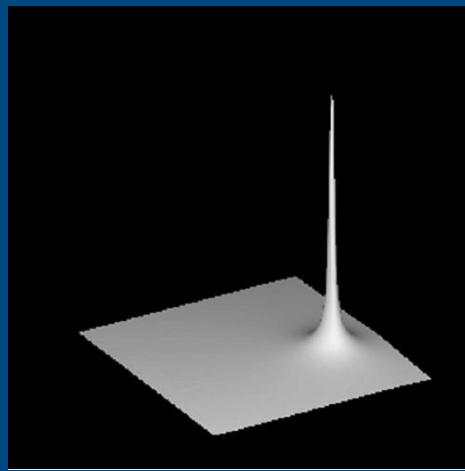
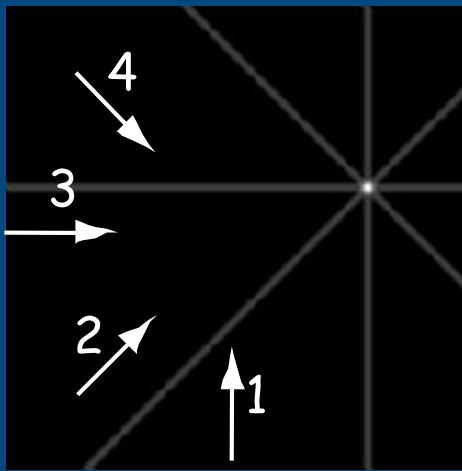
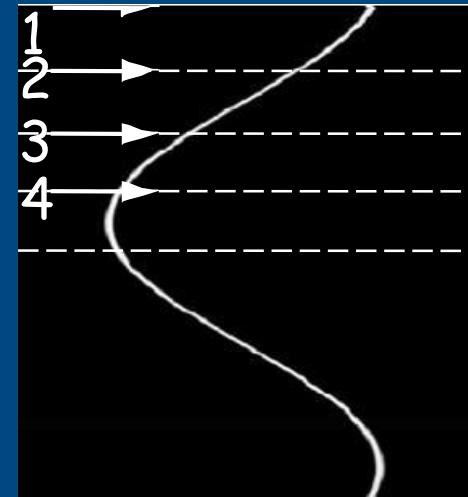
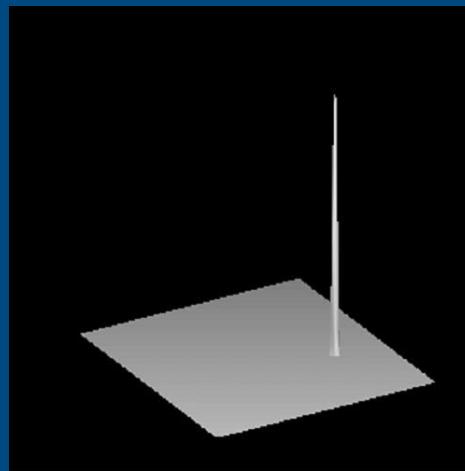
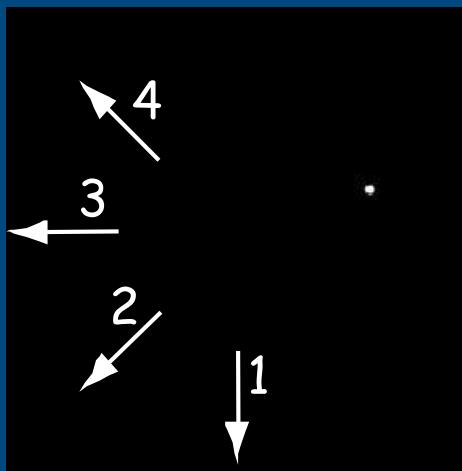
512x512 pixels
~1000 detector channels
~1000 views

250.000 unknowns
1.000.000 equations

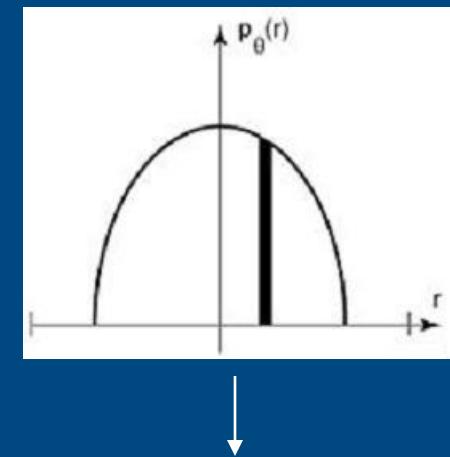
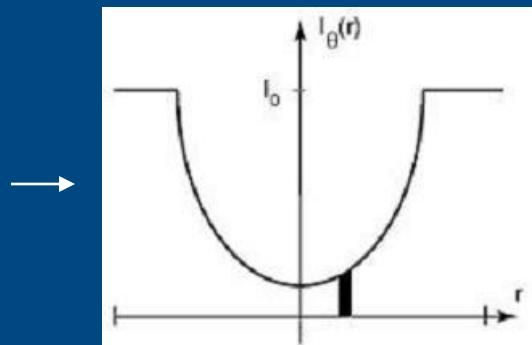
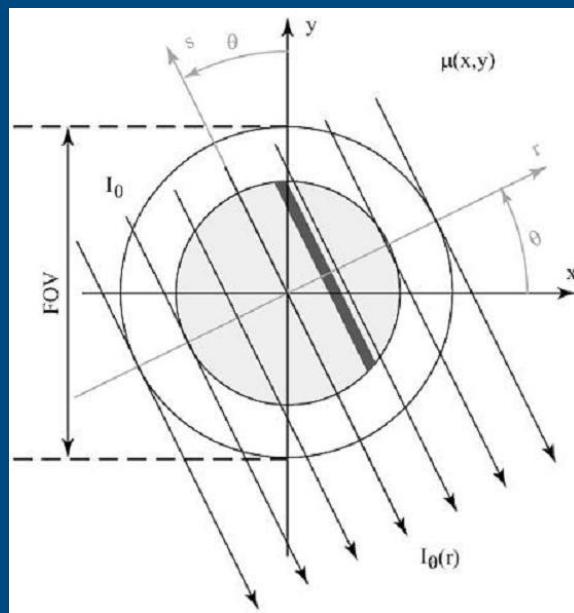
→

need practical algorithm

Backprojection



Fourier slice theorem



$$P(k, \theta) = \int_{-\infty}^{\infty} p(r, \theta) e^{-2\pi i (k \cdot r)} dr$$

$$F(k_x, k_y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-2\pi i (k_x x + k_y y)} dx dy$$

$$P(k, \theta) = F(k_x, k_y)$$

with $\begin{cases} k_x = k \cdot \cos \theta \\ k_y = k \cdot \sin \theta. \end{cases}$

Fourier slice theorem

Filtered backprojection

Direct Fourier inversion

- (1) for all θ_m (varying from 0 to π), calculate the 1D discrete FT \mathcal{F}_1 of $p(r_n, \theta_m)$ with respect to r_n :

$$\mathcal{F}_1\{p(r_n, \theta_m)\} = P(k_{n'}, \theta_m), \quad (2.25)$$

- (2) for every θ_m , put the values of $P(k_{n'}, \theta_m)$ on a polar grid,
- (3) Calculate $F(k_{x_{i'}}, k_{y_{j'}})$ (sampled on a Cartesian grid) from $P(k_{n'}, \theta_m)$, using bilinear interpolation,
- (4) and calculate the 2D inverse discrete FT \mathcal{F}_2^{-1} of $F(k_{x_{i'}}, k_{y_{j'}})$:

$$\mathcal{F}_2^{-1}\{F(k_{x_{i'}}, k_{y_{j'}})\} = f(x_i, y_j). \quad (2.26)$$

Filtered backprojection (FBP)

$$f(x, y) = \int_0^\pi \int_{-\infty}^{\infty} P(k, \theta) |k| e^{i2\pi kr} dk d\theta, \quad \text{with } r = x \cos \theta + y \sin \theta$$

Filtre HPF

16 Fixer theta: r coordonner linéaire en l'angle theta (est alpha)

k: la fréquence correspond à la coordonnée r de petit p
à grand P

Courtesy of Bruno Del Maestro GE Global Research

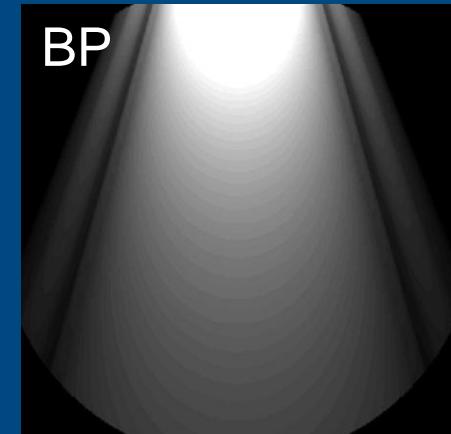
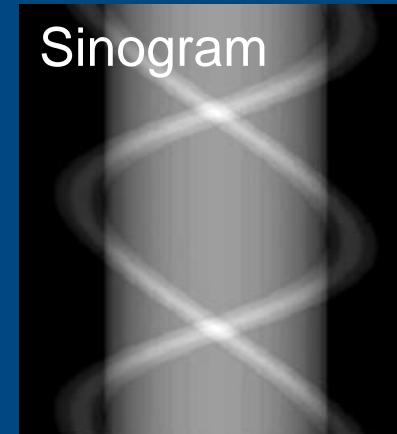
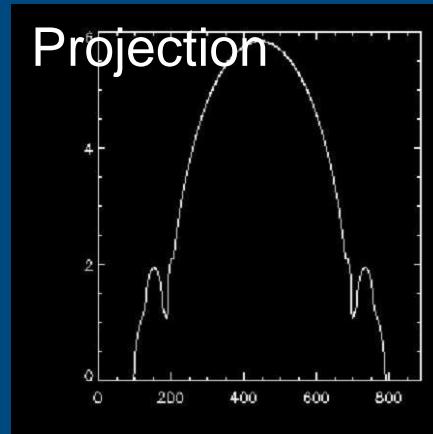
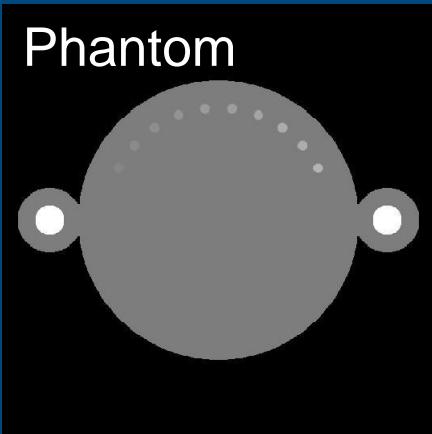
$f(t) \rightarrow F(\nu)$

$F(\nu) = \int_{-\infty}^{\infty} f(t) e^{-2\pi i t \nu} dt$

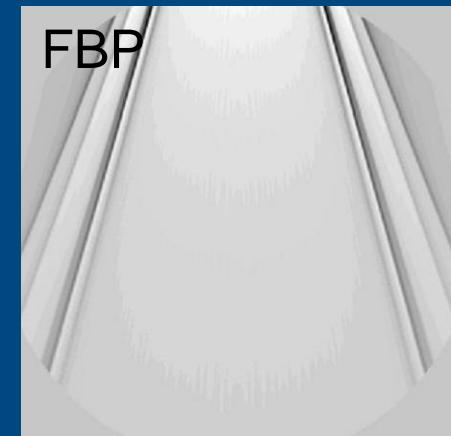
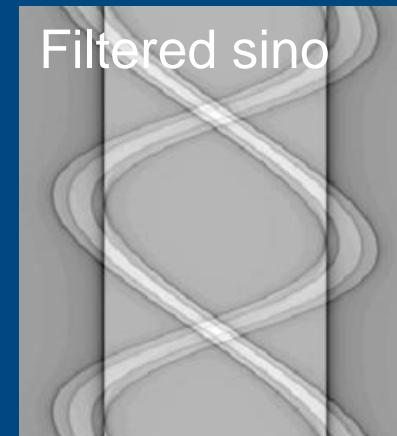
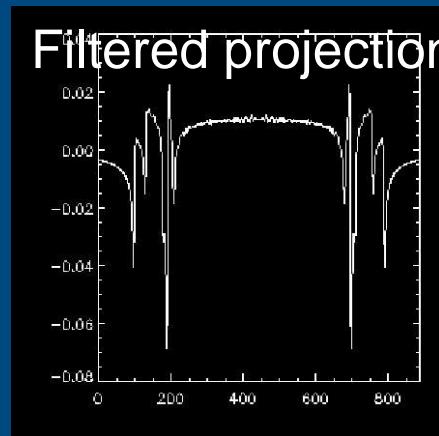
imagination at work



Backprojection - Filtered Backprojection



1 view



17 BP: Backprojection

FBP: Filtre Backprojection

HPF and Ramp PF ; filtre est necessaire pour ameliorer les images

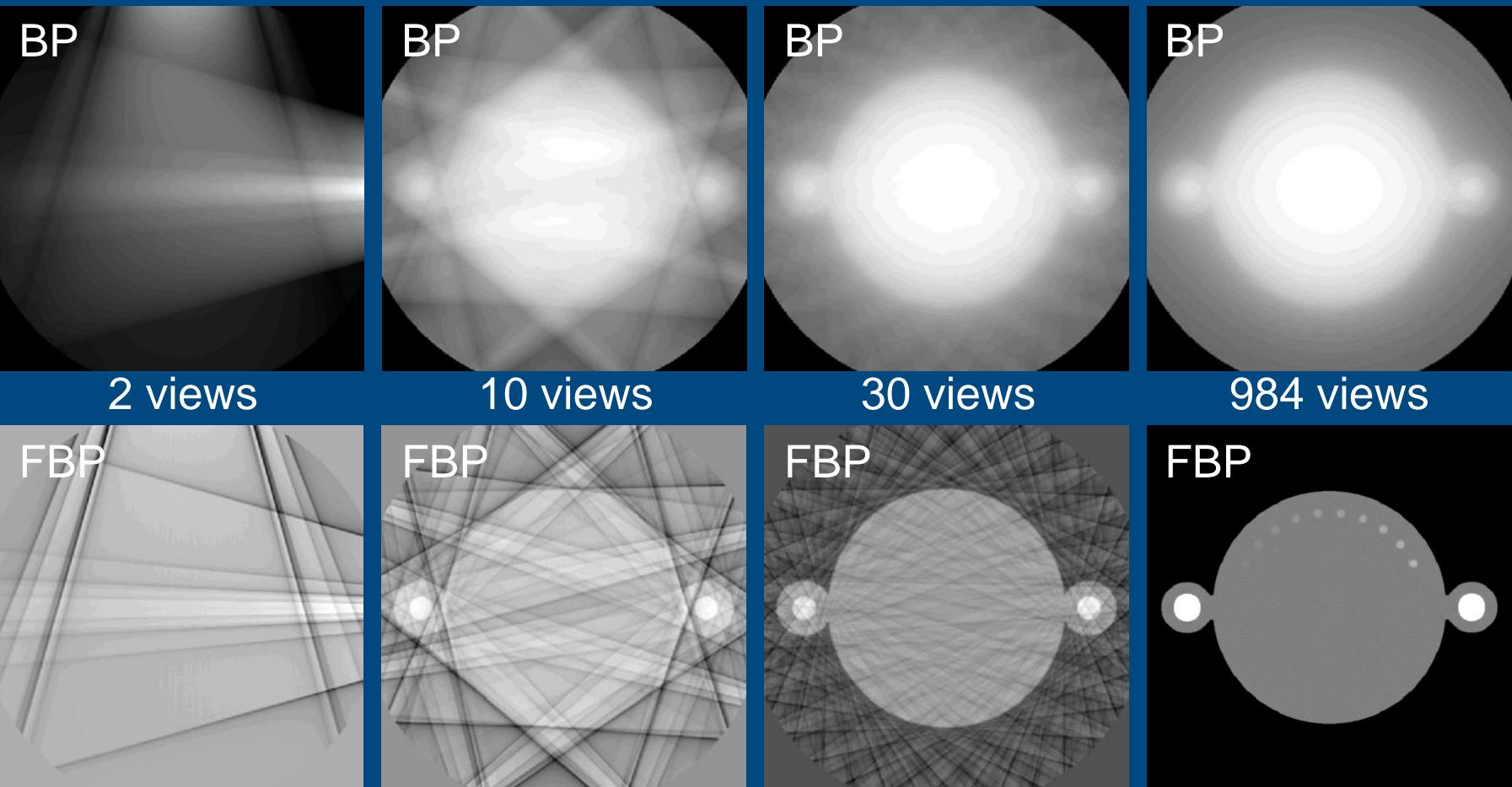
Courtesy of Bruno De Man, GE Global Research

$$P(K,\theta) = \int_{-\infty}^{+\infty} p_\theta(r) \exp(-2\pi r K) dr$$

imagination at work



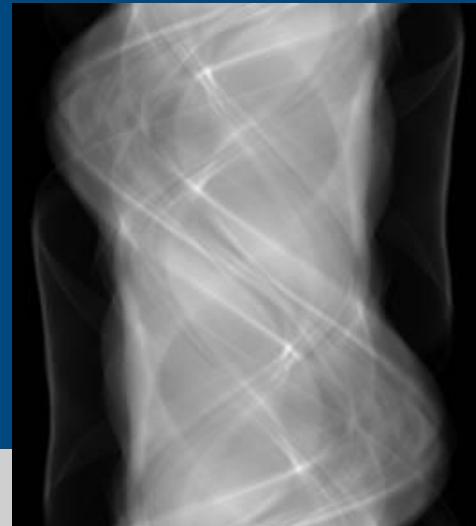
Backprojection - Filtered Backprojection



Filtered Back-projecgtion

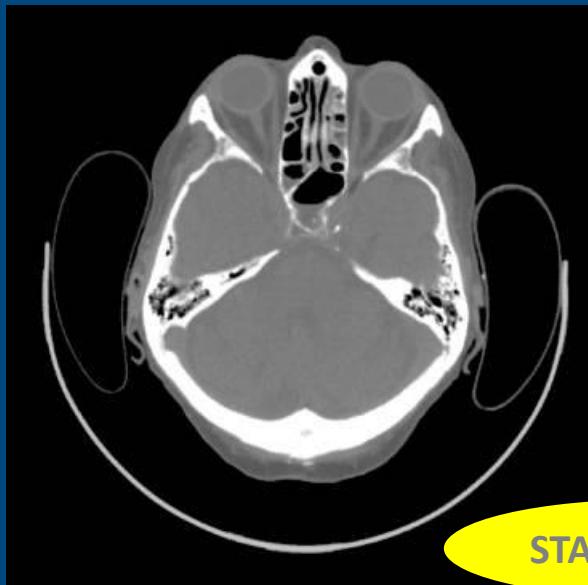


A \rightarrow



\hat{A}^{-1}

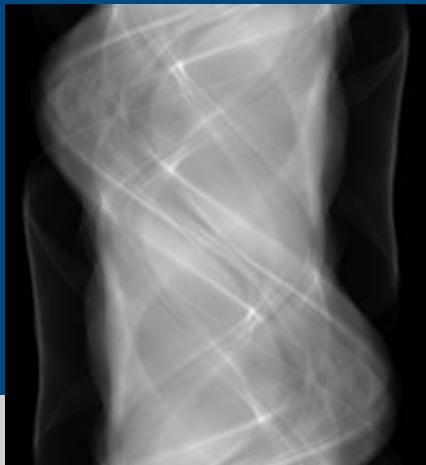
Iterative reconstruction



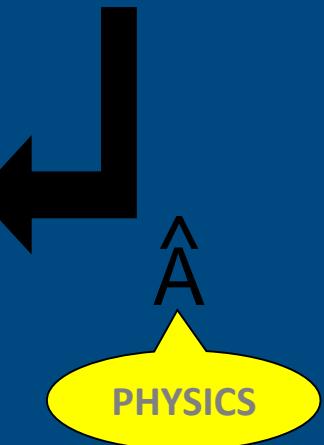
$$\hat{A}^T$$



$$L \rightarrow A$$

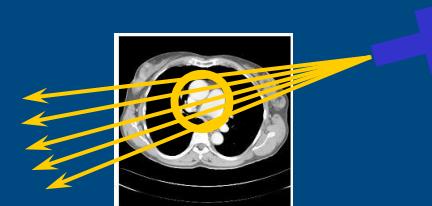
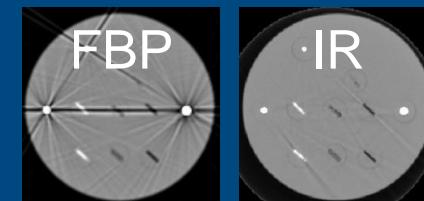
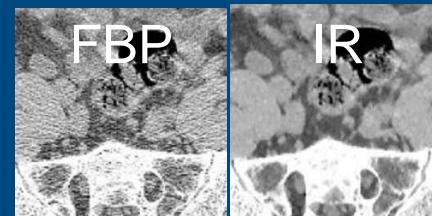


$$\hat{A}$$



Why iterative reconstruction ?

- Dose/noise reduction
- Prior information
- Missing data
 - MAR
 - Detector gaps
 - Truncation
 - Local ROI
 - Under-sampling
- Incorporate physics
- Flexibility
 - Cone-beam
 - New geometries



CT number - Hounsfield Units

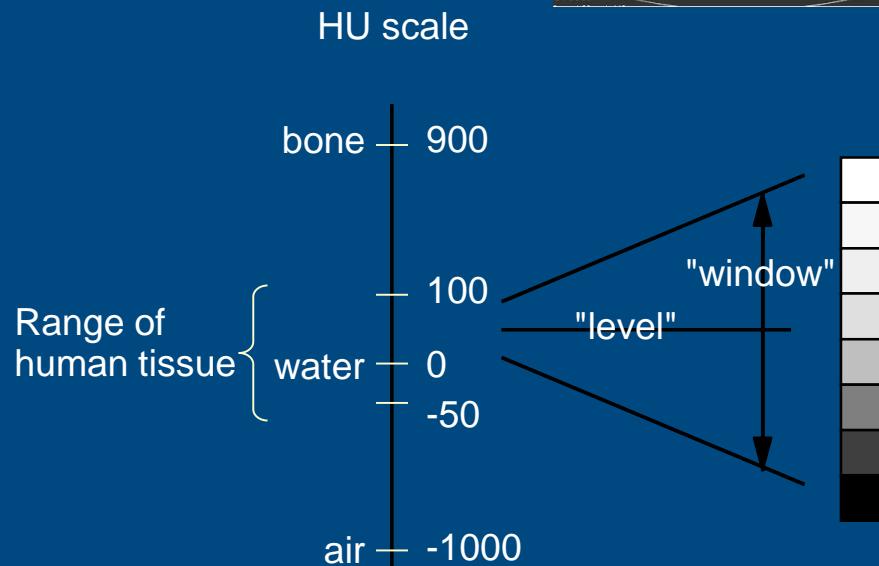
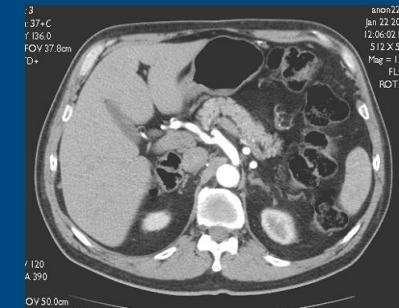
$$\text{CT number} = 1000 * (\mu - \mu_{\text{H}_2\text{O}}) / \mu_{\text{H}_2\text{O}}$$

Air = -1000 HU

Water = 0 HU

Human tissue ~ 0 HU

Bone ~ 1000HU

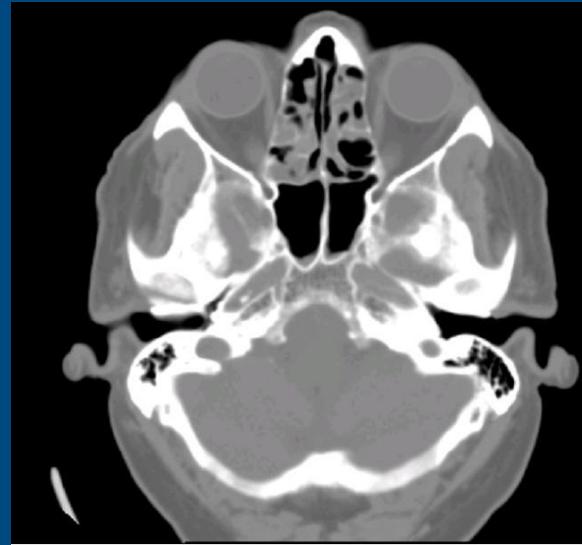


Window - level



W100, L 20

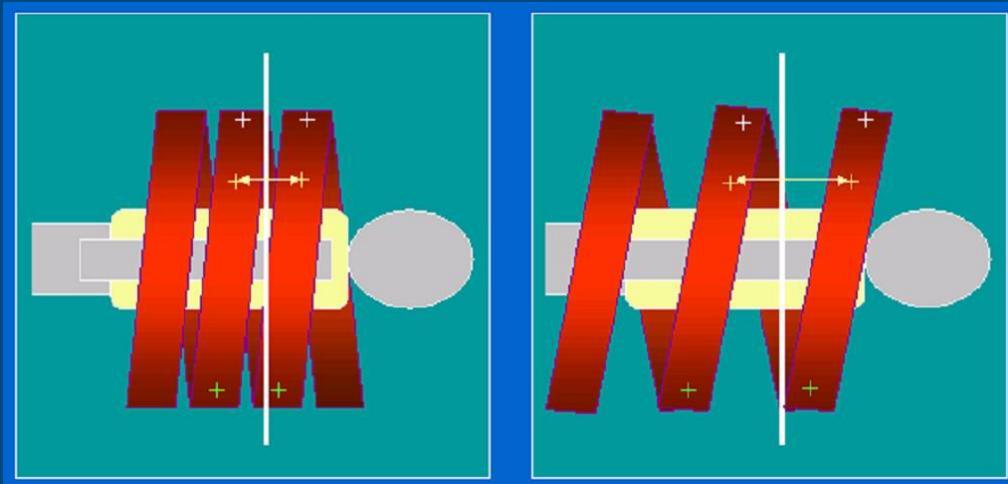
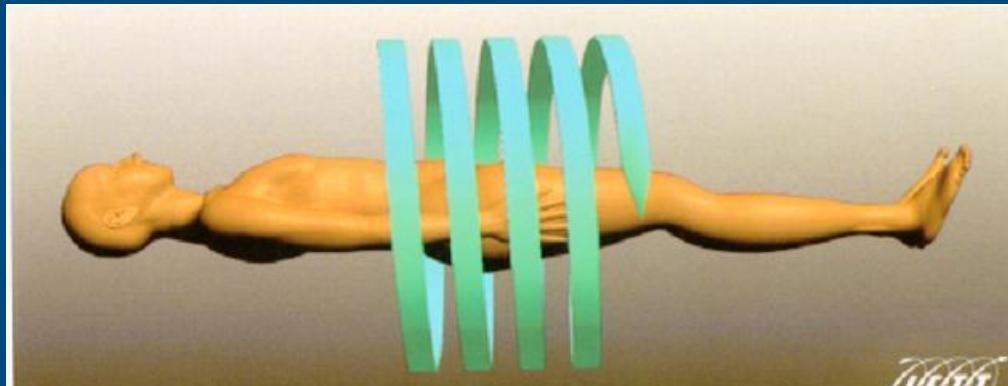
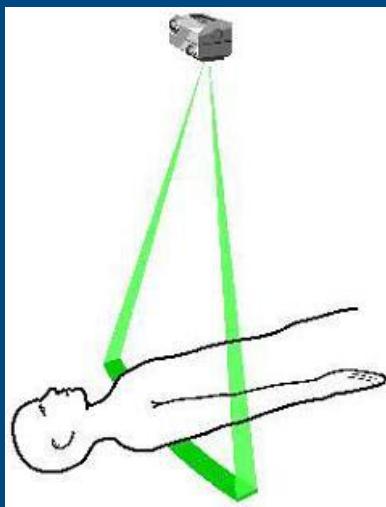
Soft tissue contrast visible



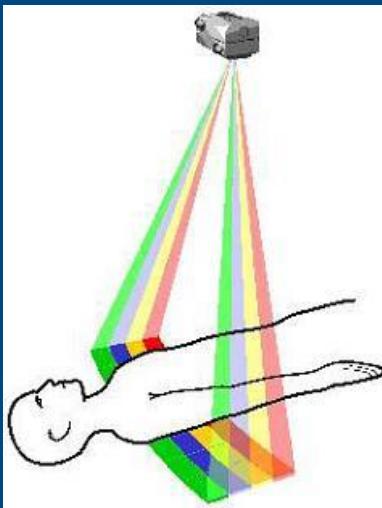
W1000, L 0

Bone structure visible

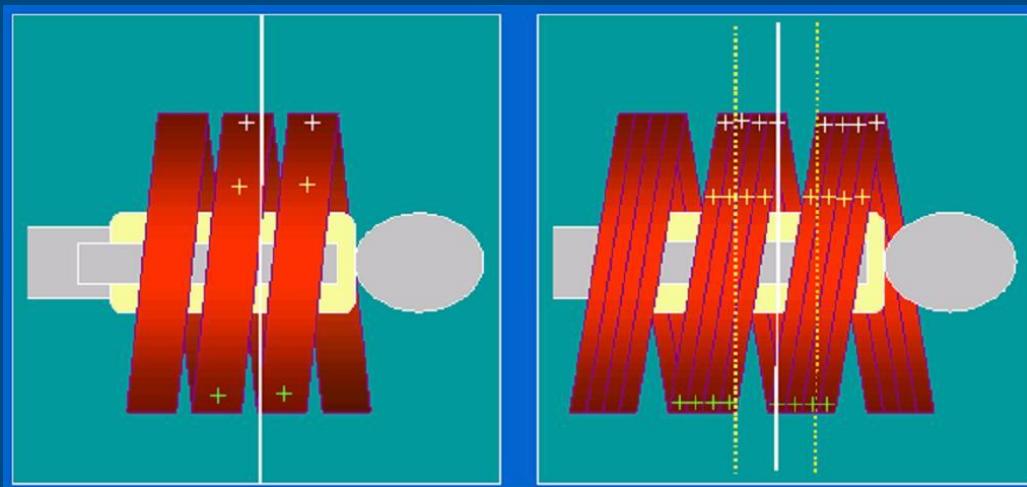
Spiral CT or Helical CT



Multi-slice CT or Multi-detector CT



Higher resolution – Larger coverage – Faster scanning



Slice wars



Manufacturer	GE	Philips	Siemens	Toshiba
CT scanner	Lightspeed 64	Brilliance 64	Sensation 64	Aquilion 64
# detector rows	64	64	32	64
row size (@iso)	0.625mm	0.625mm	0.6mm	0.5mm
total coverage (@iso)	40mm	40mm	20mm	32mm
# slices per rotation	64	64	64	64



Part I : the very very basics

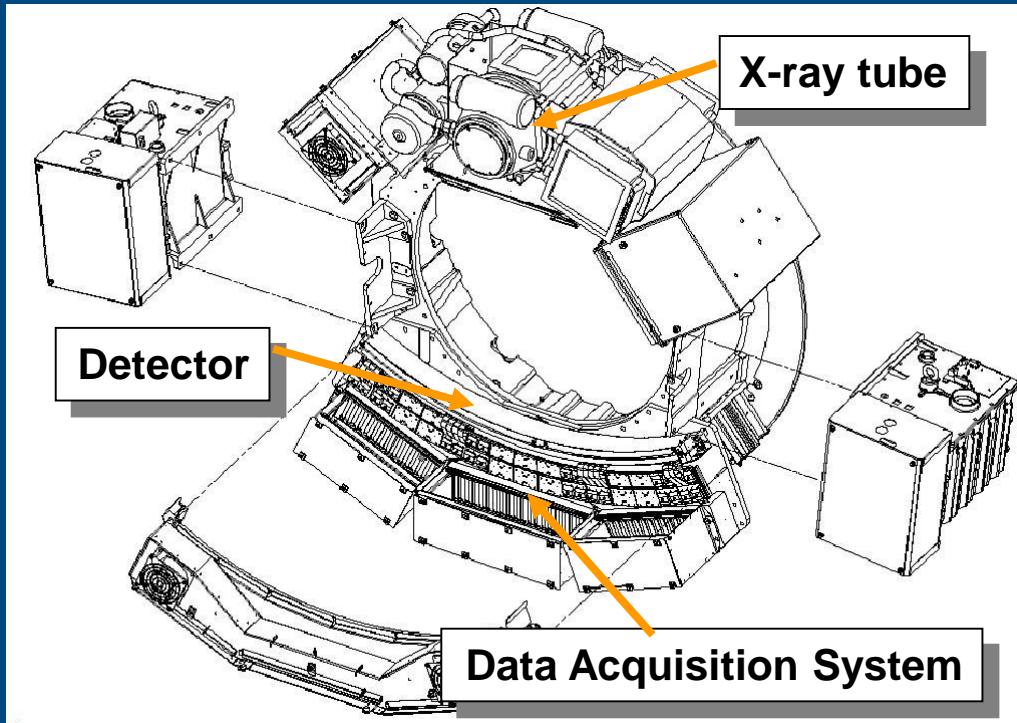
Part II : components and physics

Part III : recent advances in CT

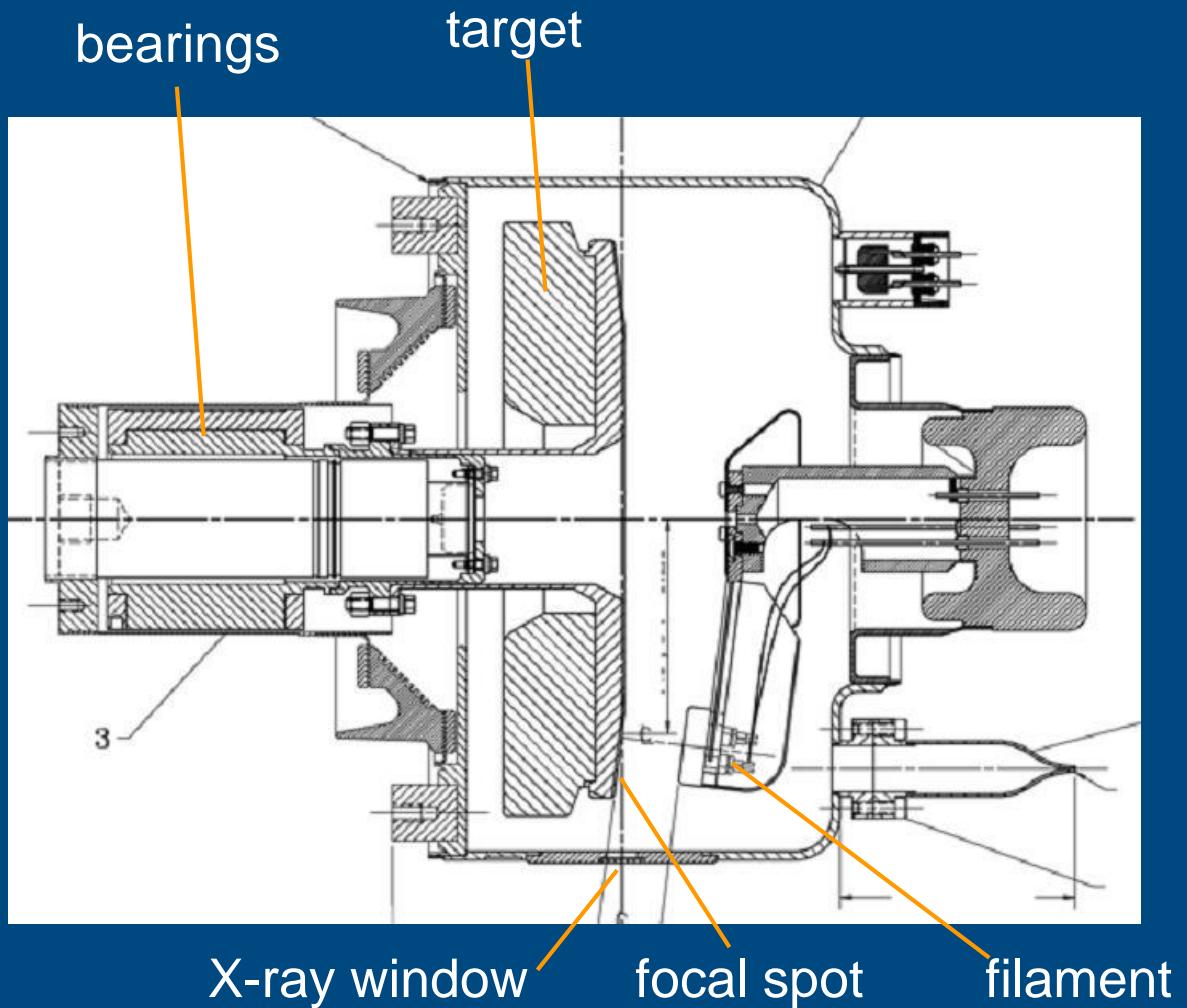
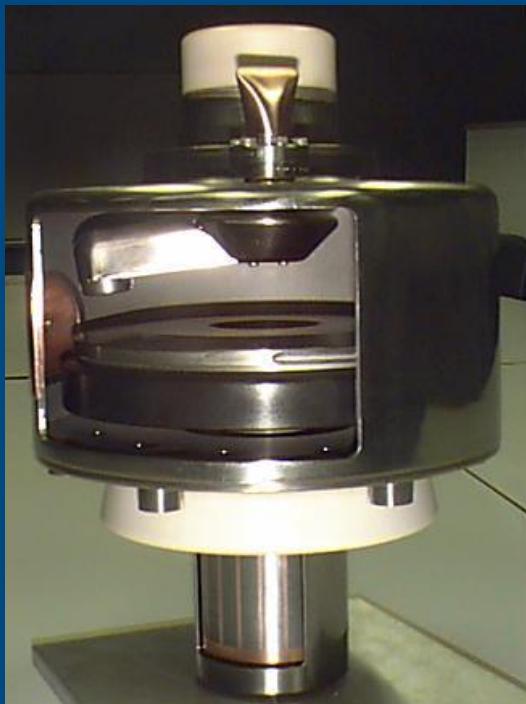
Part IV : some images



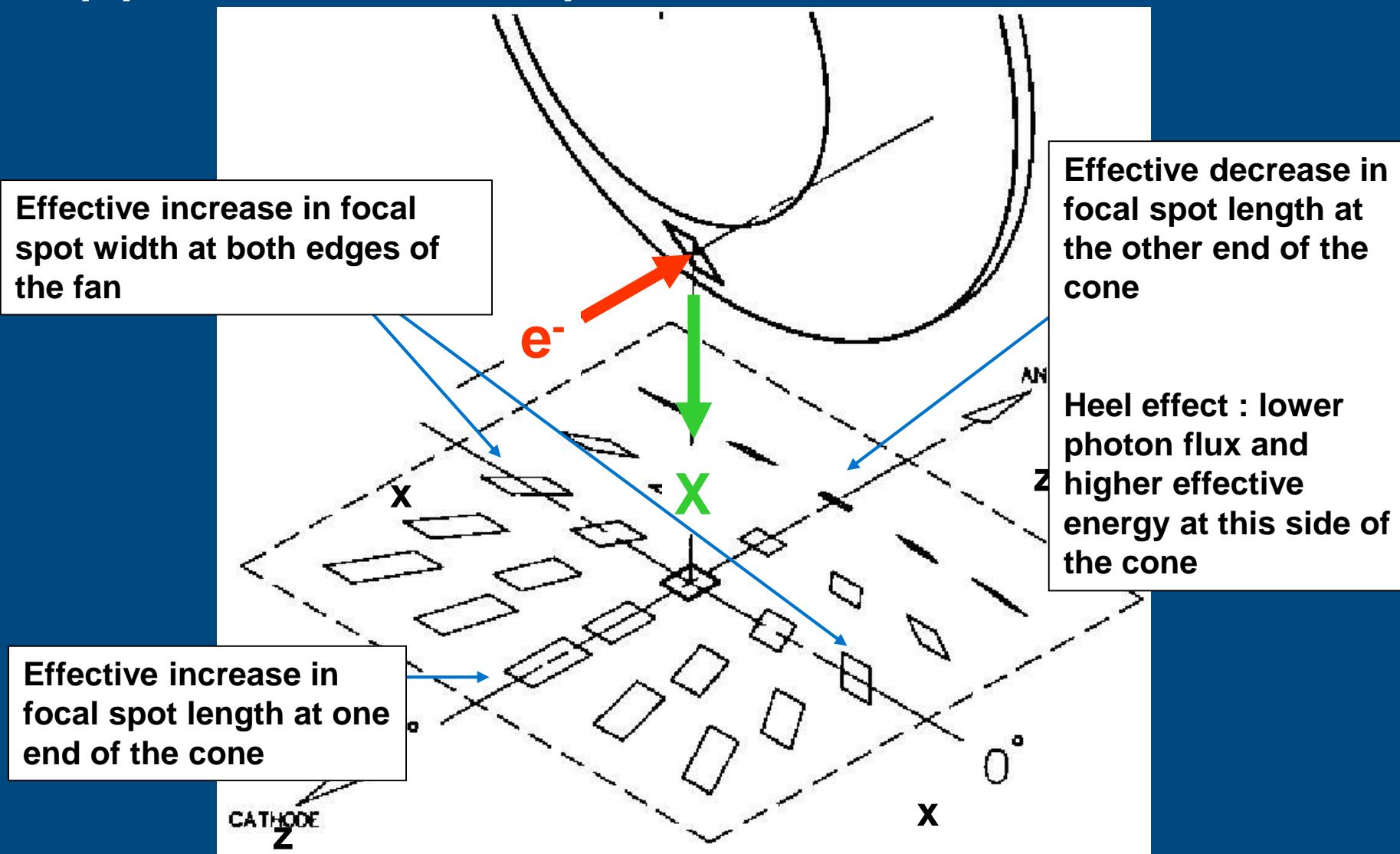
CT system and components



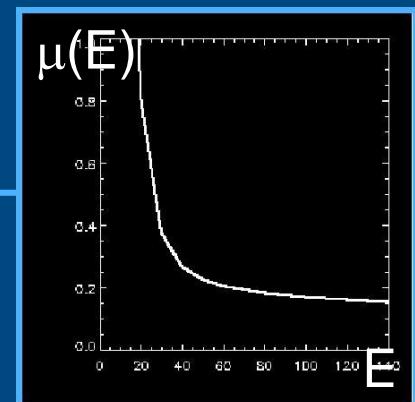
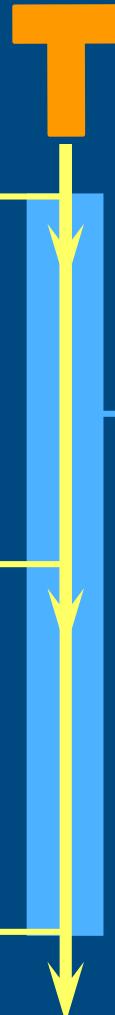
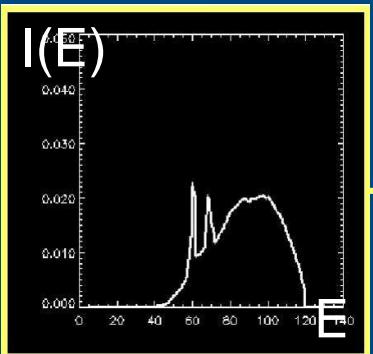
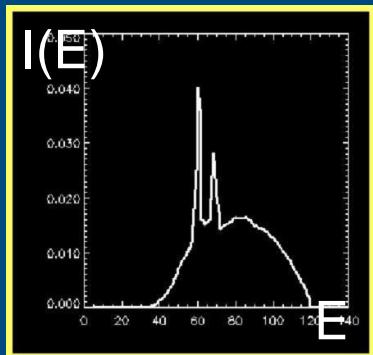
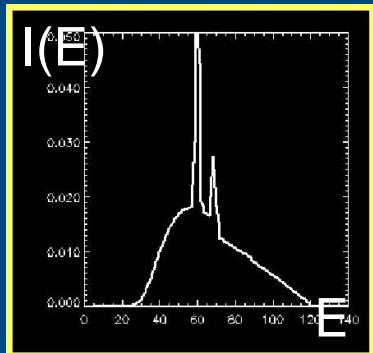
X-ray tube



Apparent focal spot size

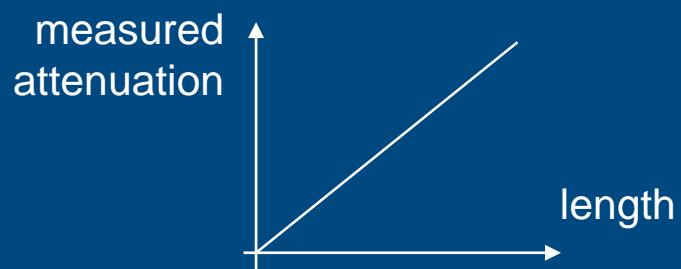
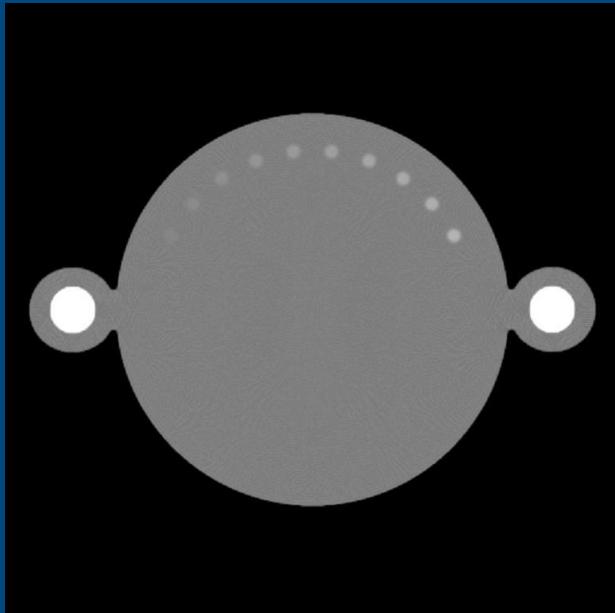


Beam hardening

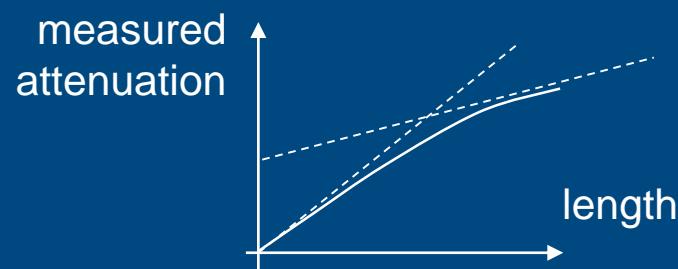
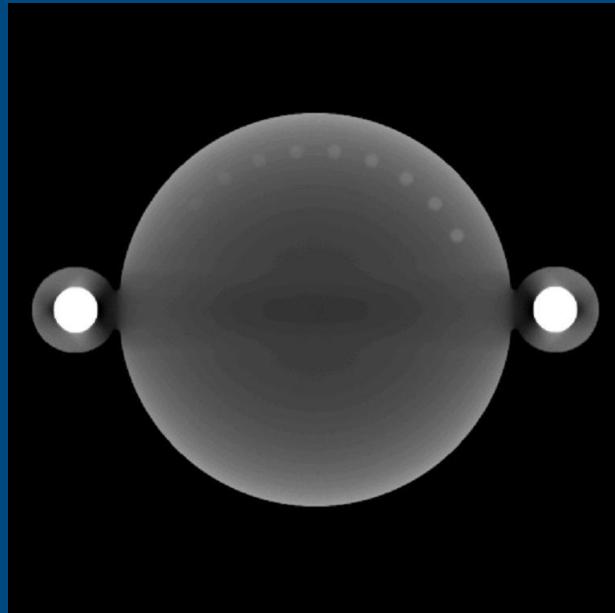


Beam hardening

Monochromatic



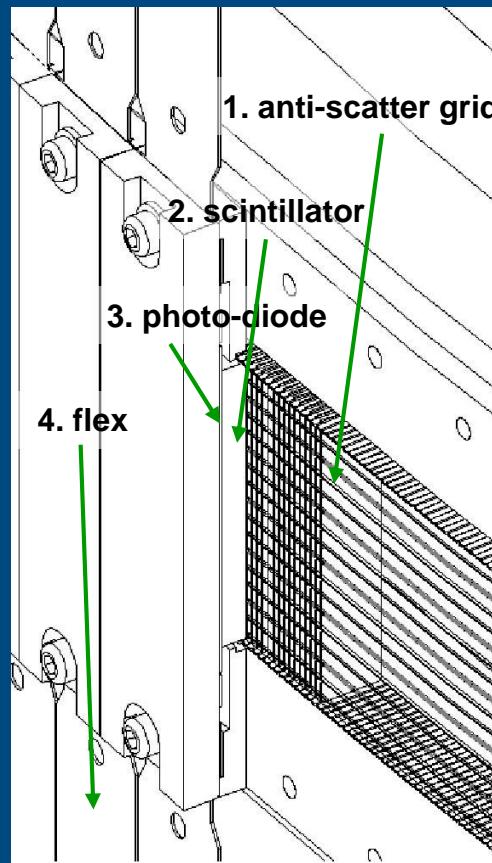
Polychromatic



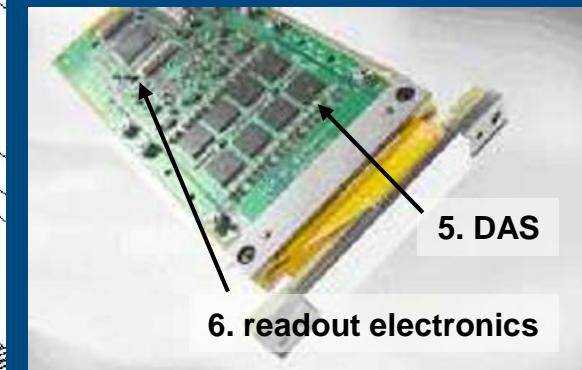
X-ray detectors



Lightspeed 16 (2002)



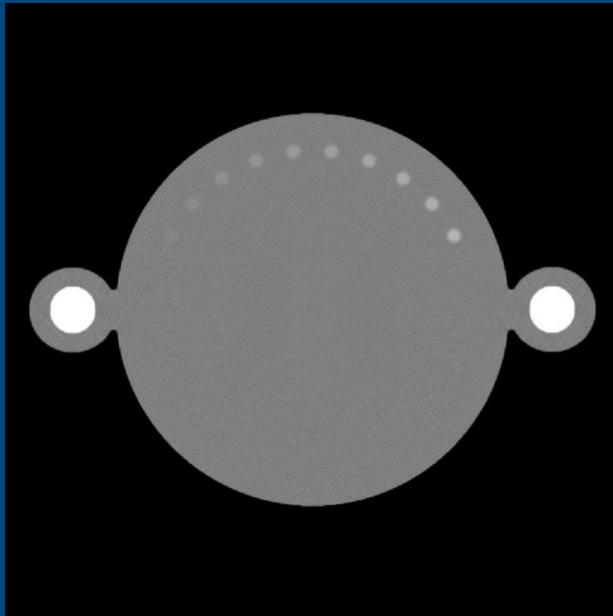
Lightspeed 16 (2002)



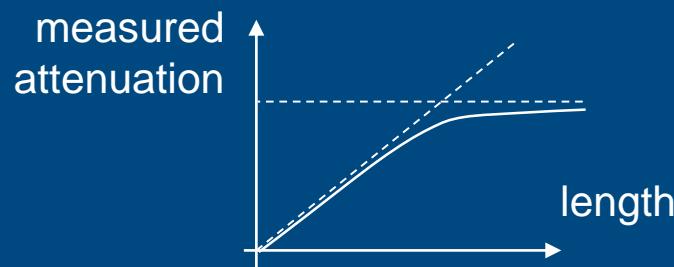
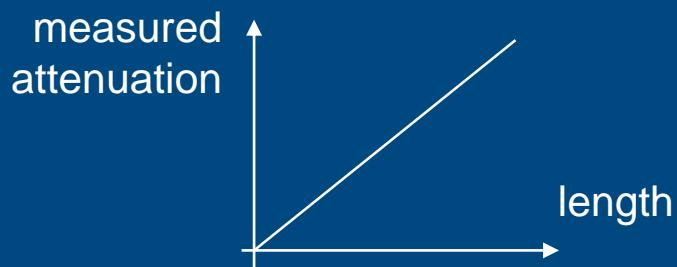
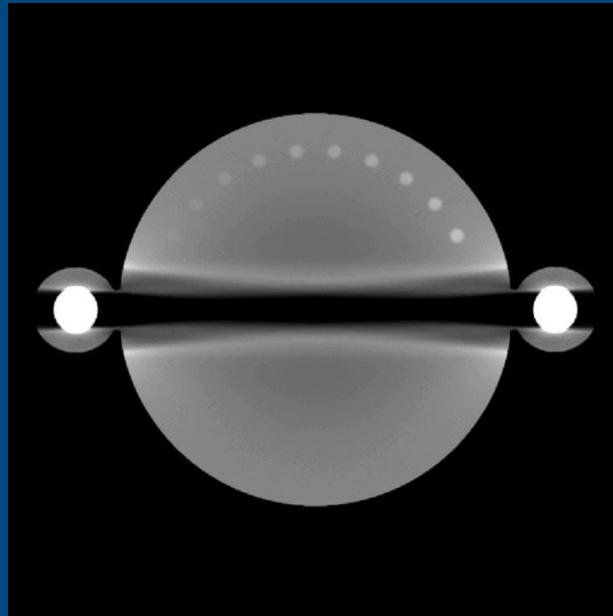
Lightspeed VCT (2004)

Scatter

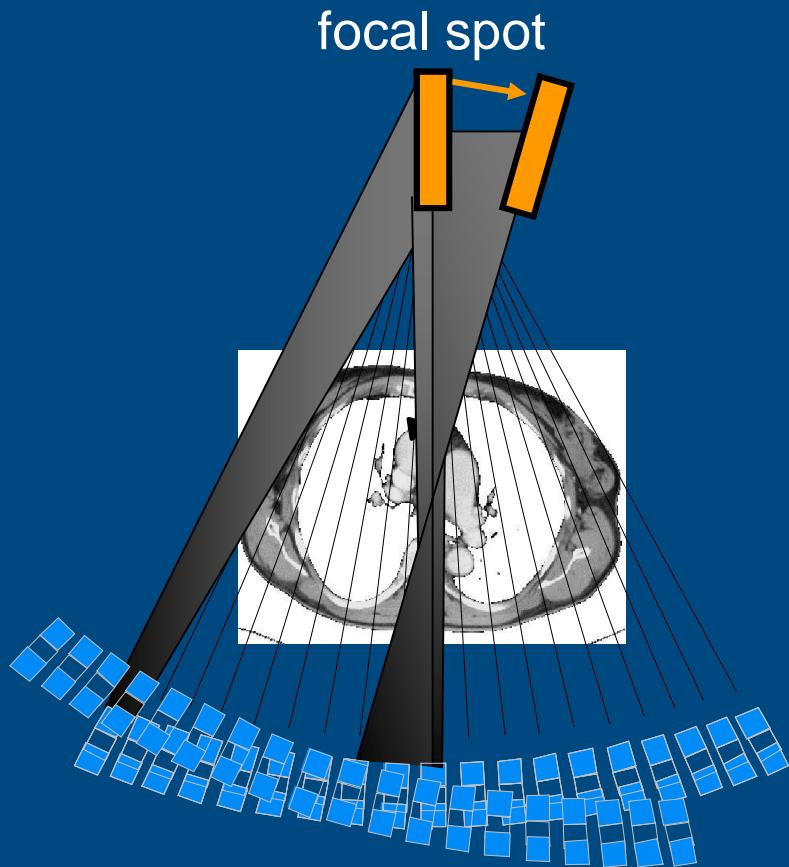
Without scatter



With scatter



Spatial resolution



Increase spatial resolution by :

- smaller detector
- smaller focal spot
- smaller detector cross-talk
- comb colimator (dose penalty!)

Uniform spatial resolution by :

- shorter focal spot
- higher number of views

Boost spatial resolution and reduce aliasing artifacts by :

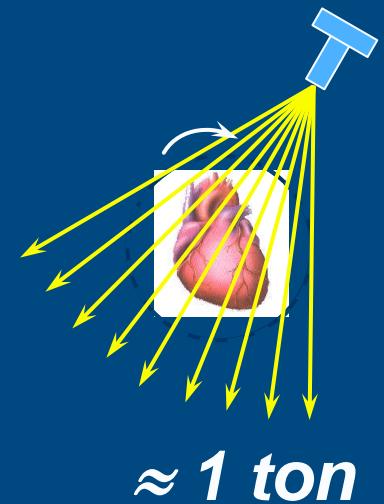
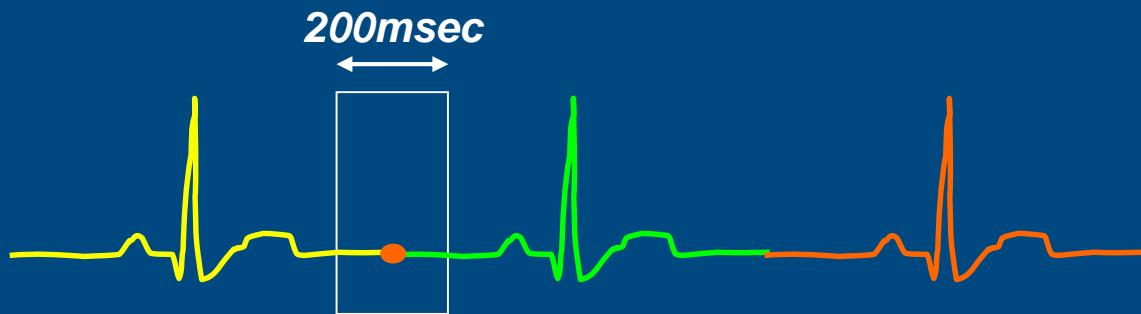
- improved interpolation / recon
- boost kernels / deconvolution
- quarter detector offset
- focal spot wobble (FFS)

Temporal resolution (cardiac CT)

rotation period : 0.35s

full-scan = $360^\circ \rightarrow$ half-scan $\approx 230^\circ$

temporal resolution : 200ms



Cardiac CT: multi-sector recon

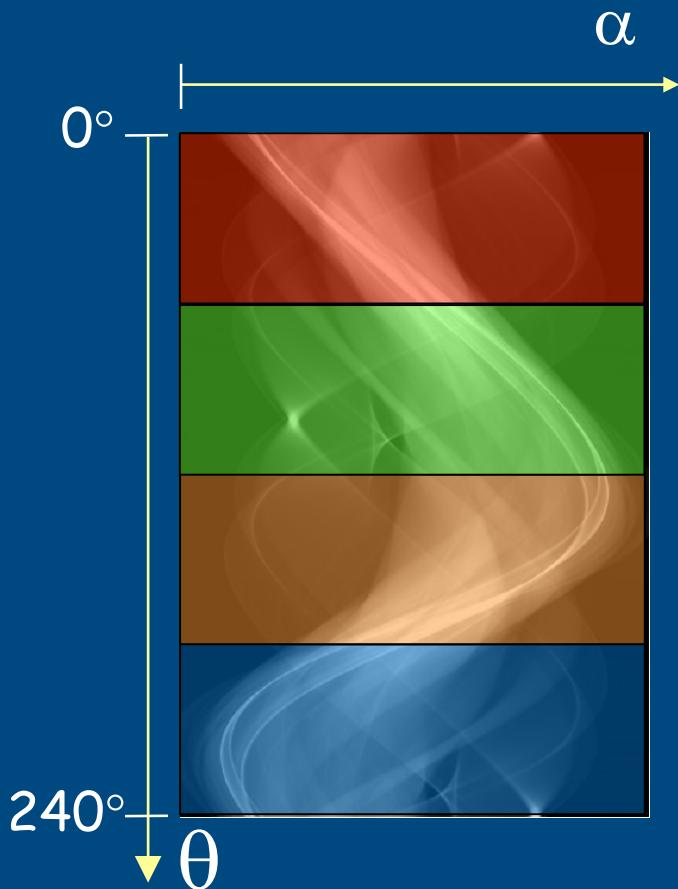
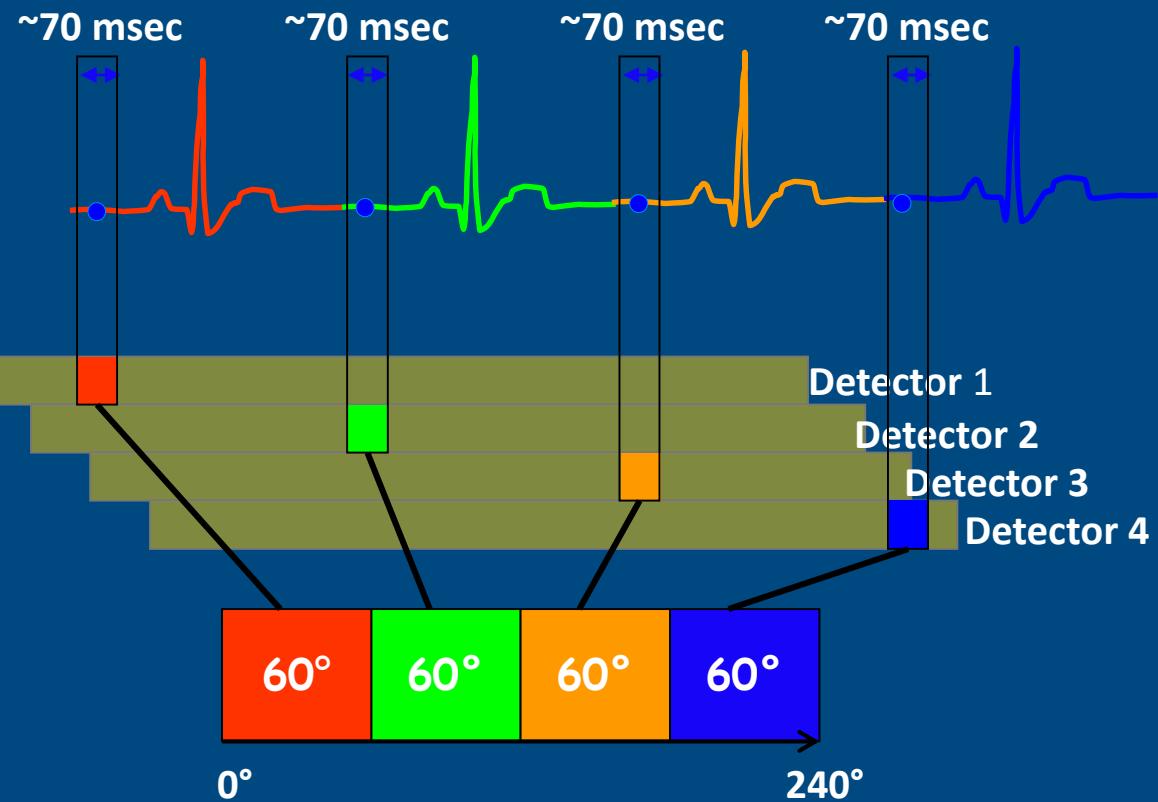
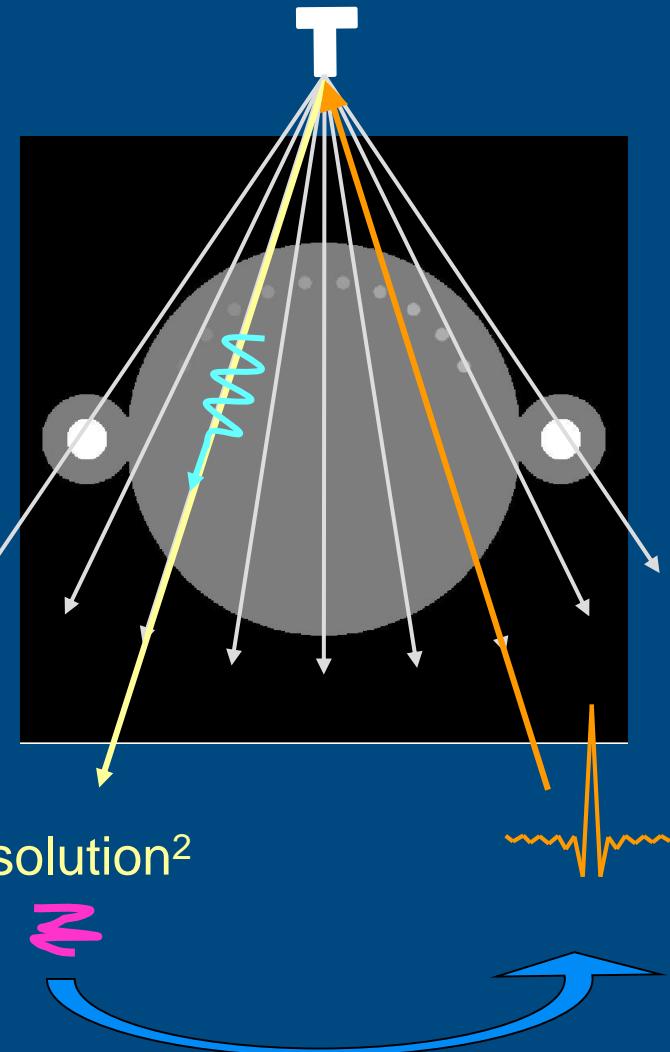


Image noise

Sources :

- quantum noise
(X-rays)
- electronic noise
(detector)



$$\sigma_p \sim \exp(p/2) / \sqrt{I_0} \cdot \text{resolution}^2$$

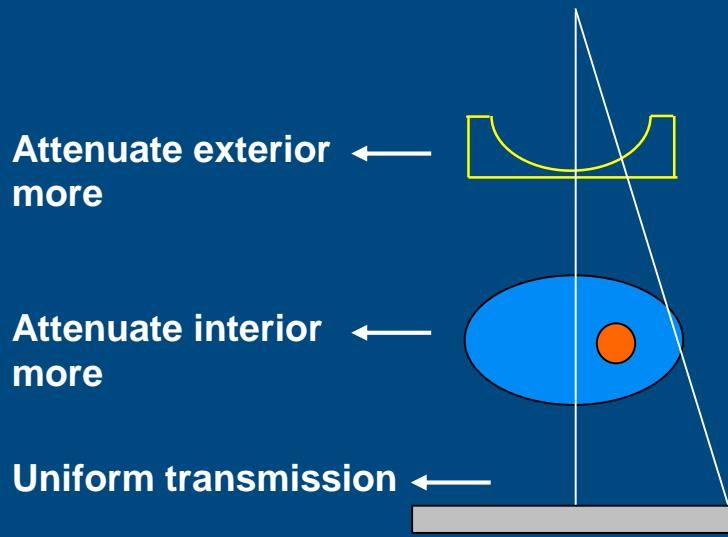
ζ

ζ

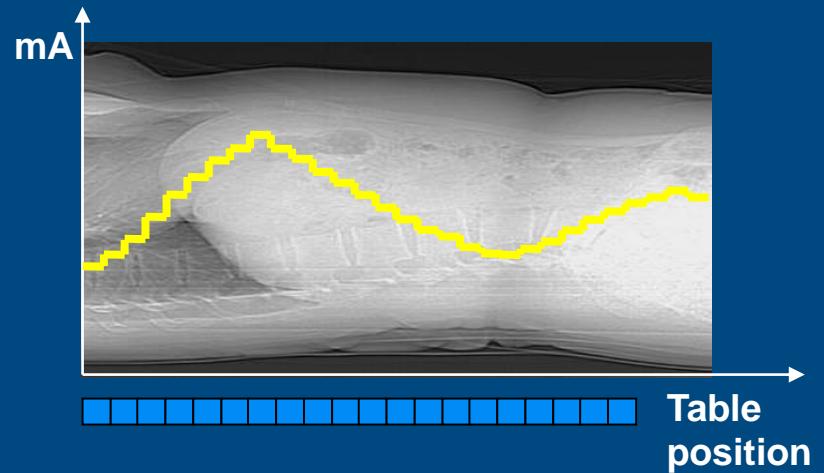
ζ

Optimizing dose-efficiency

Bow-tie filter



Tube current modulation (auto-mA)



Part I : the very very basics

Part II : components and physics

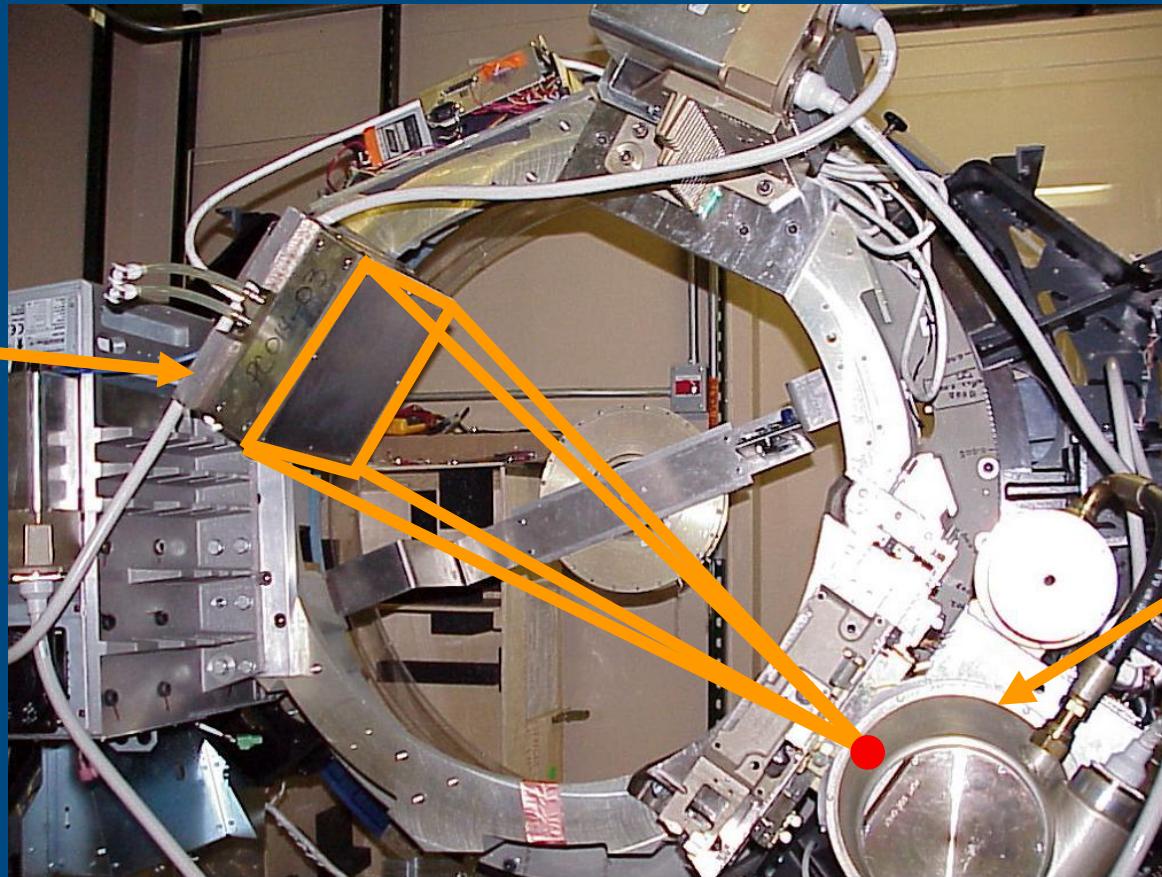
Part III : recent advances in CT

Part IV : some images



Flat-panel hi-res VCT

flat-panel
detector :
1024x360
channels



x-ray
tube

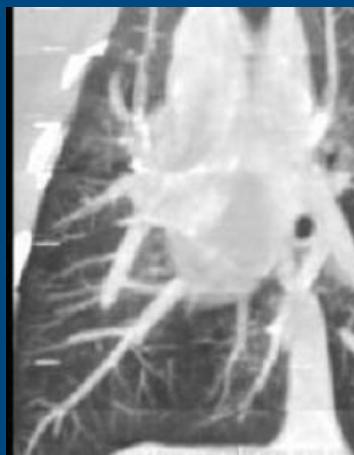
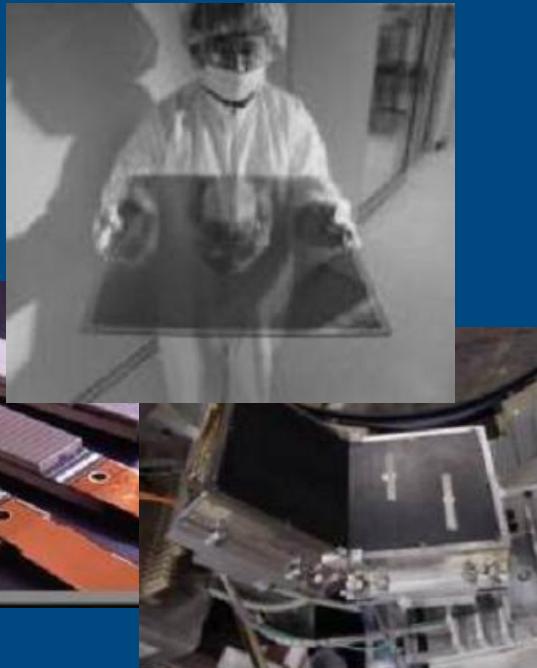
Flat-panel hi-res VCT

2001	2002	2003	2004
<ul style="list-style-type: none">• 1-panel sys• Hi-res• Limited FOV• Algorithm Investigation	<ul style="list-style-type: none">• 2-panel sys• Hi-res• Extended FOV• Further Algorithm Investigation	<ul style="list-style-type: none">• 3 Units<ul style="list-style-type: none">• MD Anderson• U Giessen• Goettingen U• 500+ Studies• Apps Research	<ul style="list-style-type: none">• 4-panel sys• Large FOV



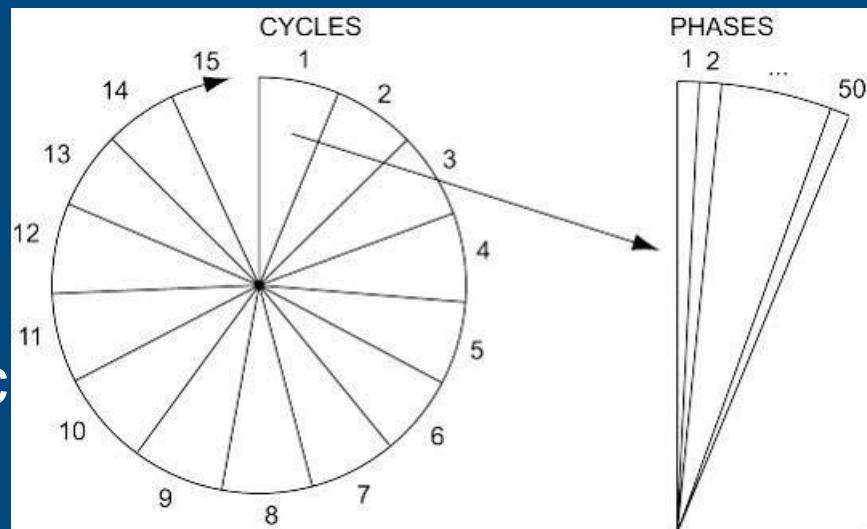
JUSTUS-LIEBIG-
UNIVERSITÄT
GIESSEN

THE UNIVERSITY OF TEXAS
MD ANDERSON
CANCER CENTER



Slow-gantry cardiac CT

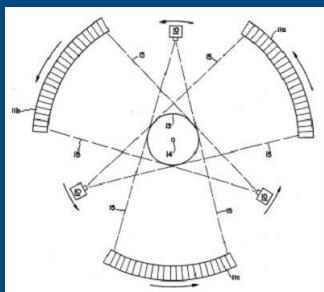
- 1 full rotation
- 18s acquisition
- 1500 views
- 180bpm (rabbit heart)
- 1 heart cycle = 1/3sec
- 54 heart cycles
- 28 phases / cycle
- temp.res. ~ 12ms



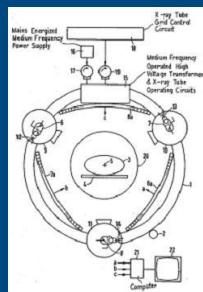
Slow-gantry cardiac CT



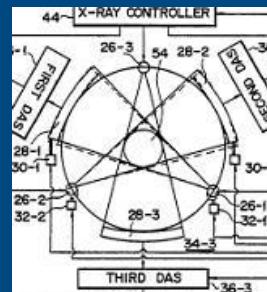
Multi-tube multi-detector CT



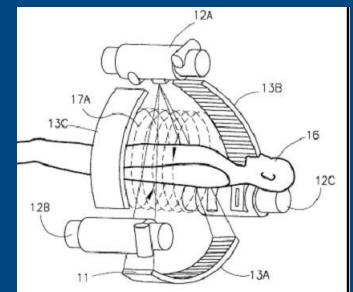
GE 1980



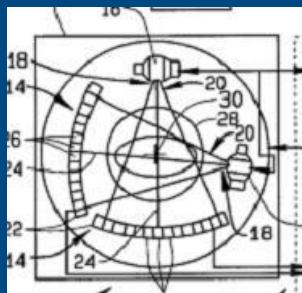
Siemens 1983



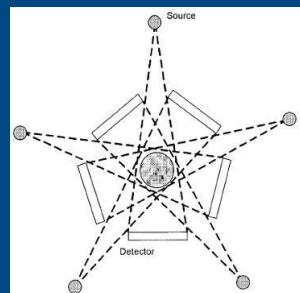
Toshiba 1991



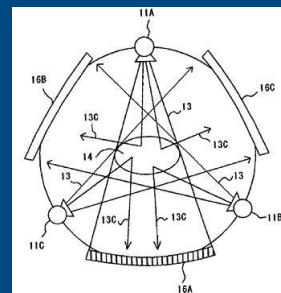
Picker 1999



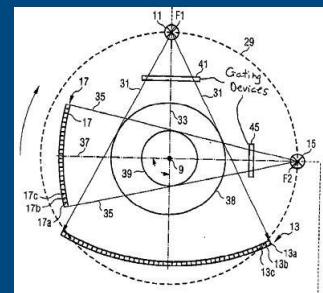
GE 2002



Wang 2002



Toshiba 2004



Siemens 2004

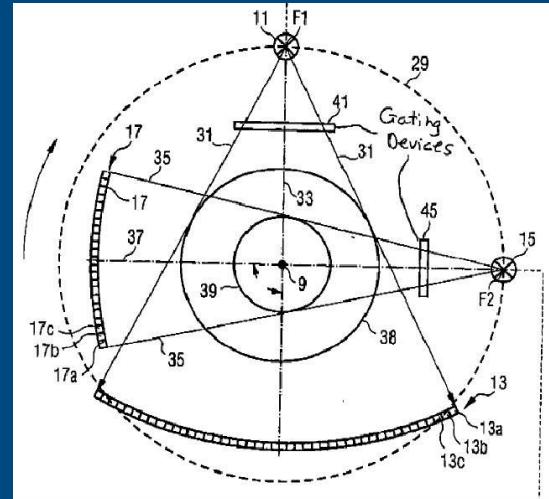
Multi-tube multi-detector CT

Benefit :

- 120° half-scan (i.s.o. 210°)

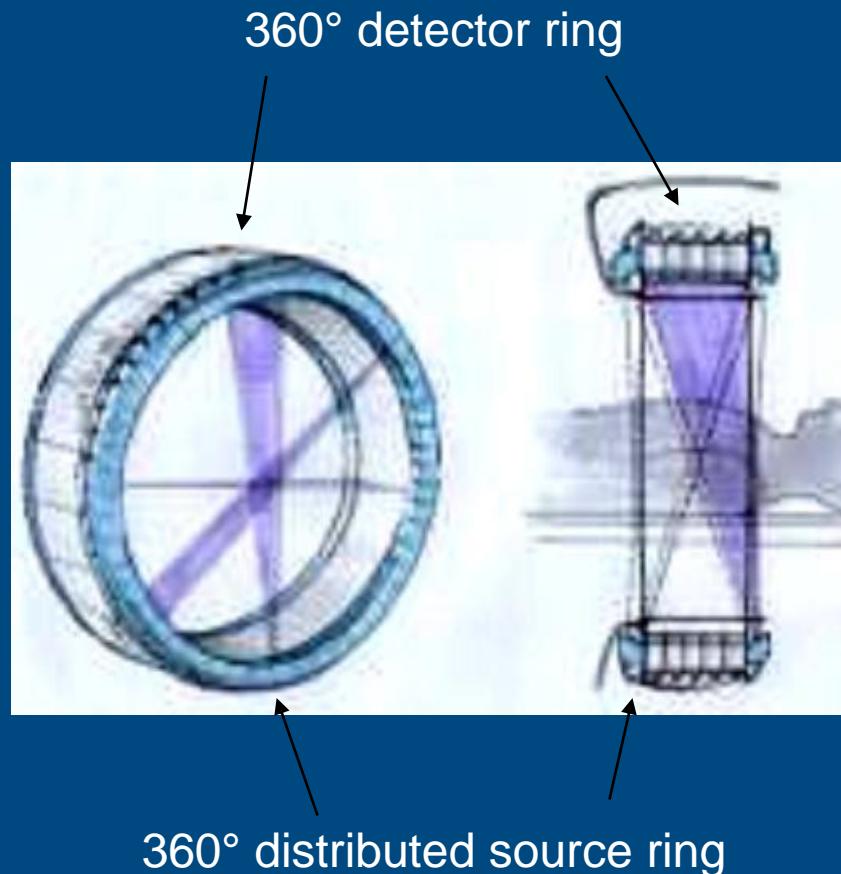
Challenges :

- Cross-scatter
- Size / weight / cost

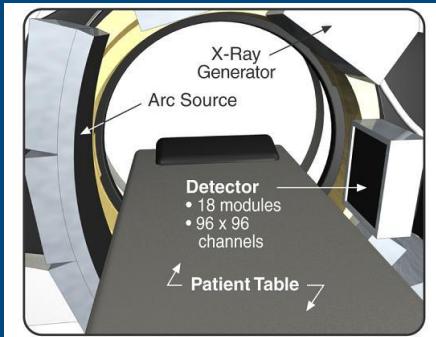


	2 x 50kW tube 2 x 20mm detector	1 x 100kW tube 1 x 40mm detector
Coverage	20mm	40mm
Temporal res	120° or 210°	210°
Power	50kW or 100kW	100kW
Dual kVp	50kW @ 1 rot.	100kW @ 2 rot.
Scatter	↑↑↑	=

Stationary CT (a.k.a. SCT)

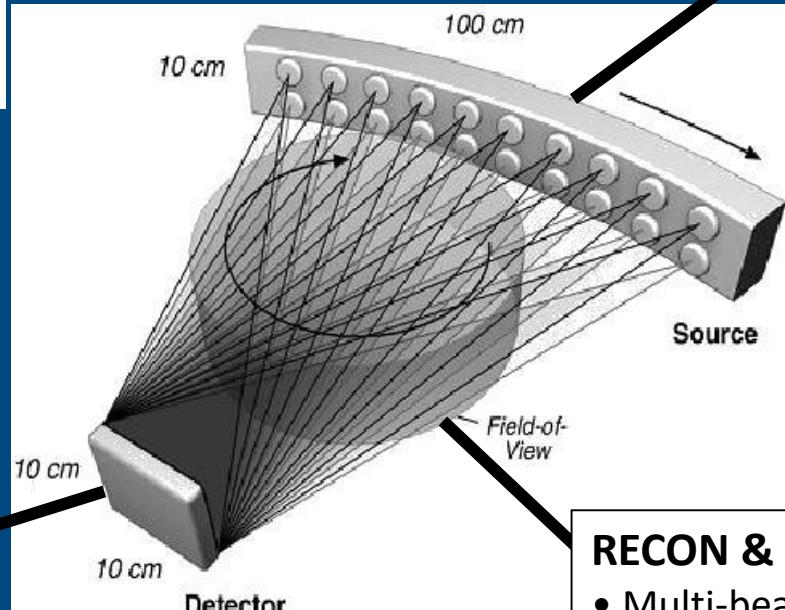


Multi-source inverse-geometry CT



X-RAY SOURCE

- 1 vacuum vessel
- multiple spots in-plane
- multiple spots in z
- solid-state e⁻-emitters
- fast sequencing
- small fan-angles
- mA modulation



DETECTOR

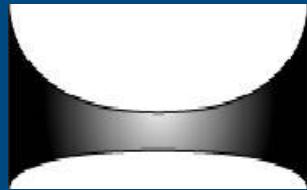
- small flat-panel
- high frame rate
- photon-counting
- small cell size
- no scatter grid

RECON & CAL

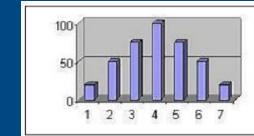
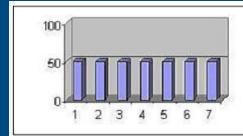
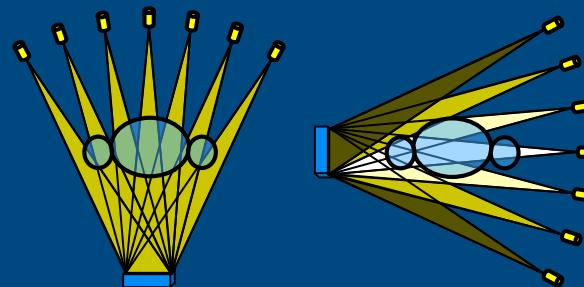
- Multi-beam rebinning
- Multi-axial cone-beam recon
- Low-dose statistical recon
- Multi-beam calibration

Virtual bowtie

Conventional bowtie



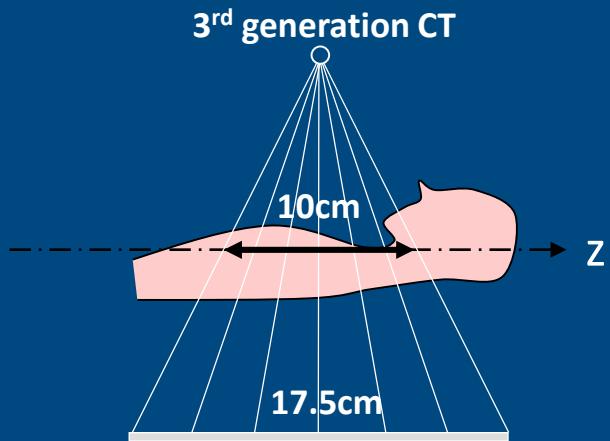
- absorbs large x-ray fraction
- shape fixed



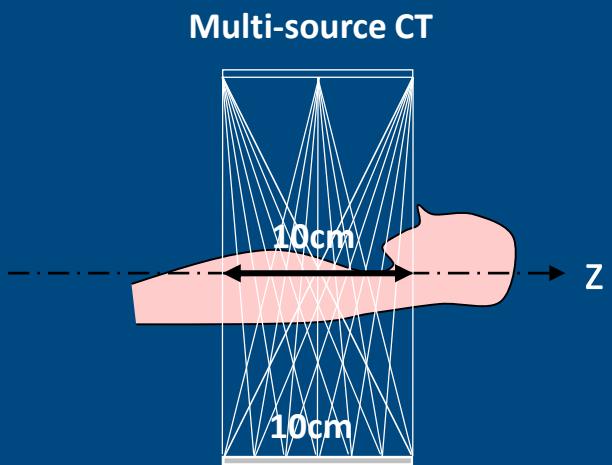
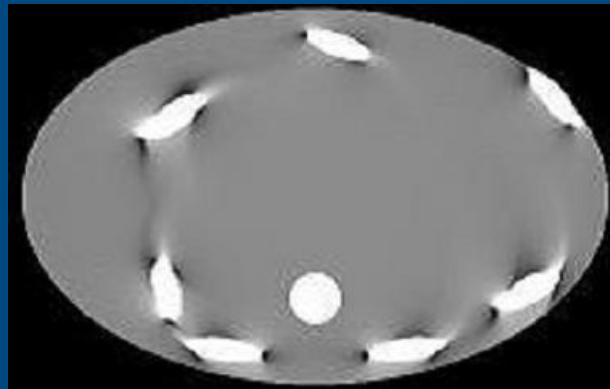
- reduced dose @ fixed noise
- reduced noise @ fixed dose
- improved (?) noise structure



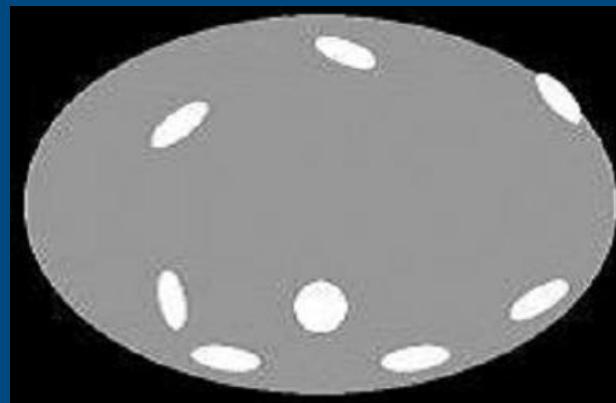
Volumetric coverage & cone-beam artifacts



10cm - 3rd generation CT

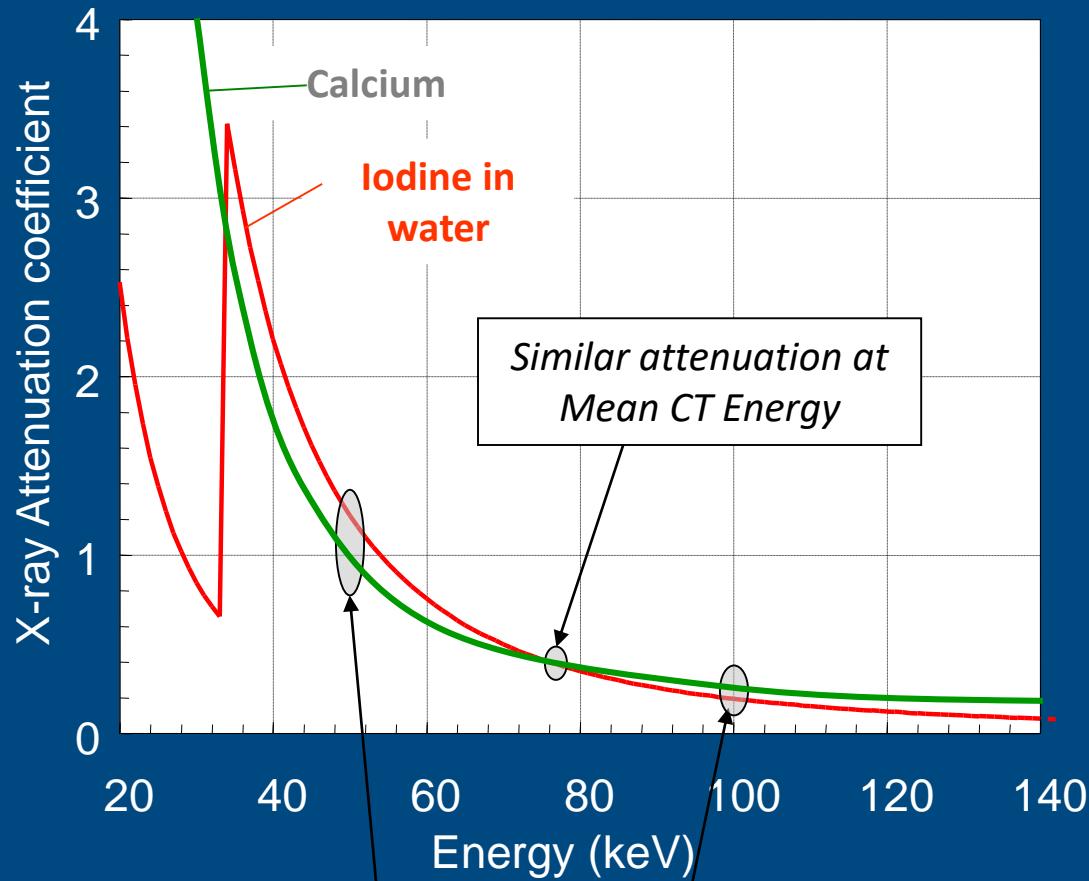


10cm - Multi-source CT



Spectral CT

- Photon-counting
- Dual kVp (short-term)
- Dual layer (worst --> Philips)

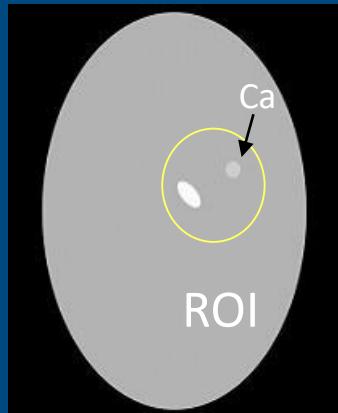


Differentiate materials through the energy dependence of the attenuation curve



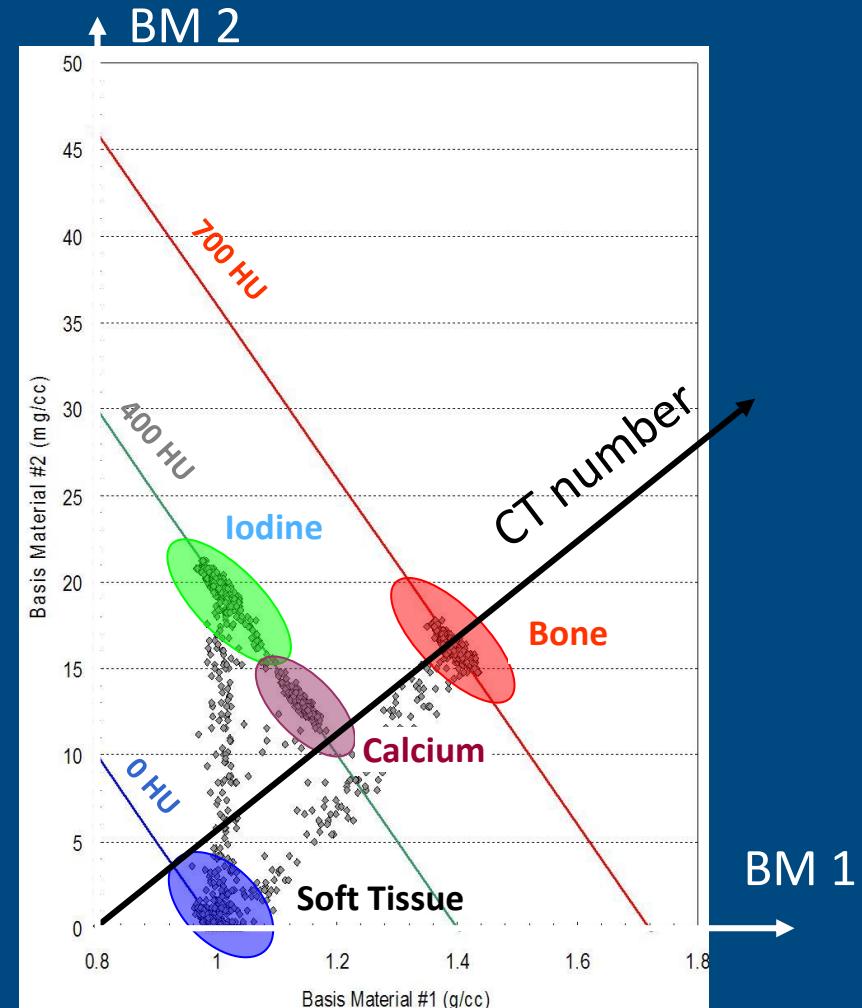
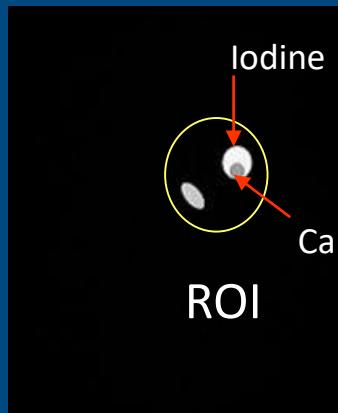
Dual kVp CT

“Soft Tissue”
Image
 (“Basis Material #1”)



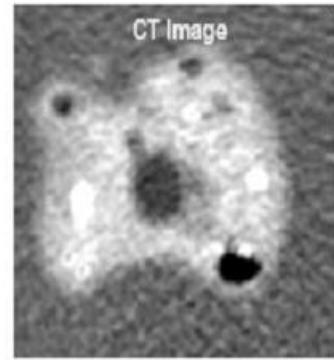
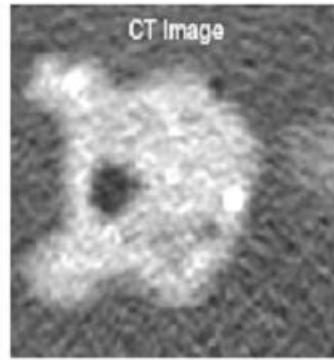
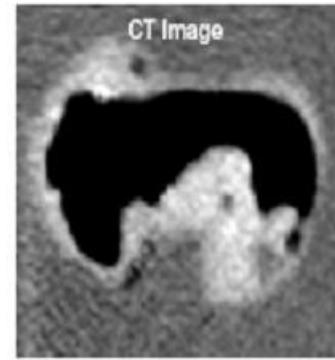
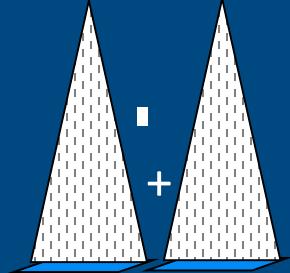
Dual kVp
acquisition and
reconstruction

“Iodine” Image
 (“Basis Material #2”)

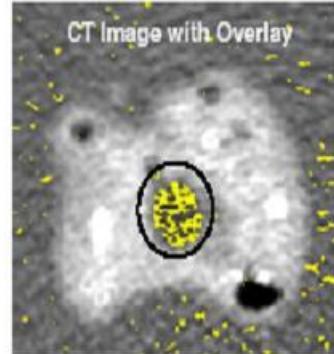
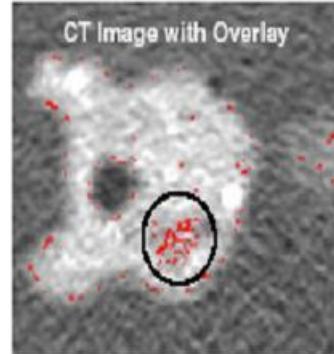
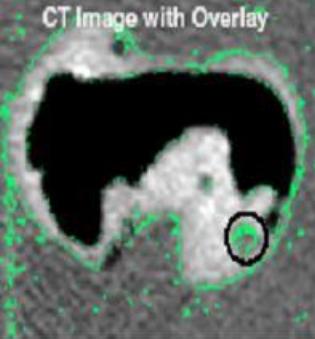
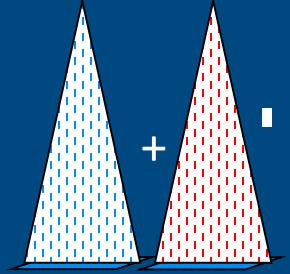


Dual kVp CT : virtual colonoscopy

120kVp 120kVp



80kVp 140kVp

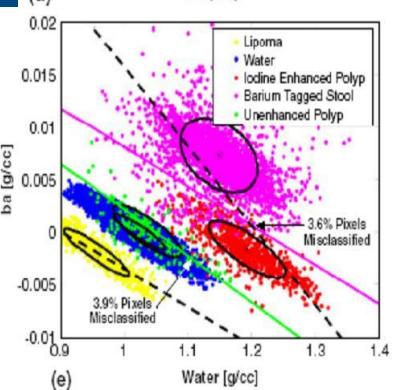
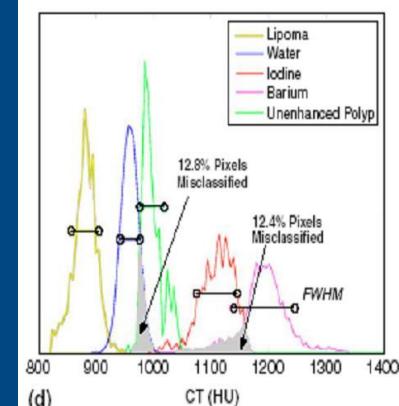


(a) Unenhanced Polyp

(b) Iodine Enhanced Polyp

(c) Lipoma Tumor

Lipoma
Water
Iodine
Barium
Unenhanced Polyp



Part I : the very very basics

Part II : components and physics

Part III : recent advances in CT

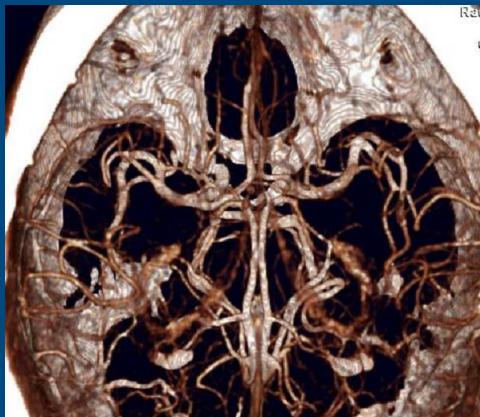
Part IV : some images



Clinical applications : head



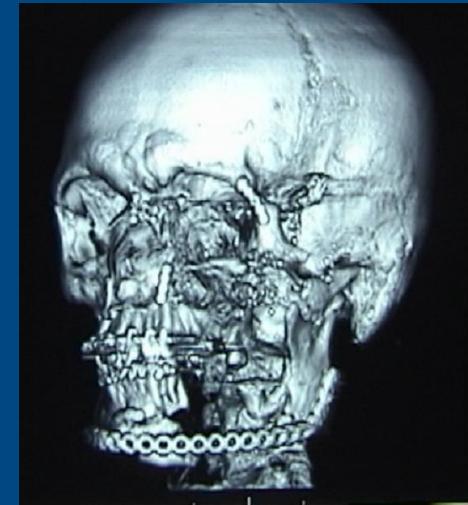
Routine head
Perfusion (stroke)



Circle of Willis

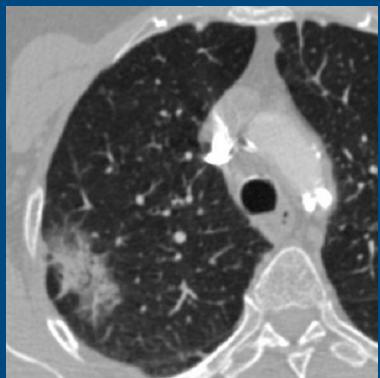


Sinuses



Trauma
temporal bone
Facial bones

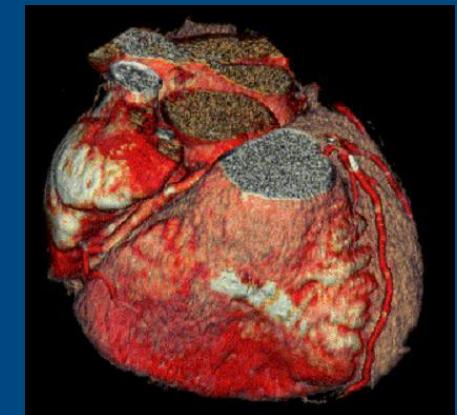
Clinical applications : oncology & cardiac



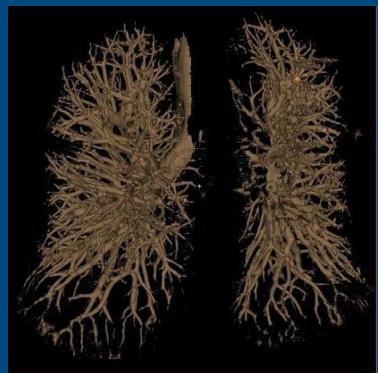
Lung nodules
Diffuse lung disease



CT Colonography for
Cancer detection



Stenosis / re-stenosis
Calcium scoring



Clinical applications : abdominal

Dual or tri phase liver

Pancreas

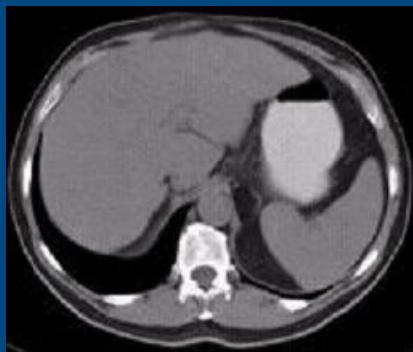
Kidney studies

Adrenals

Pelvis

Trauma

Advanced Apps: Perfusion, colonography



Clinical applications : orthopedics

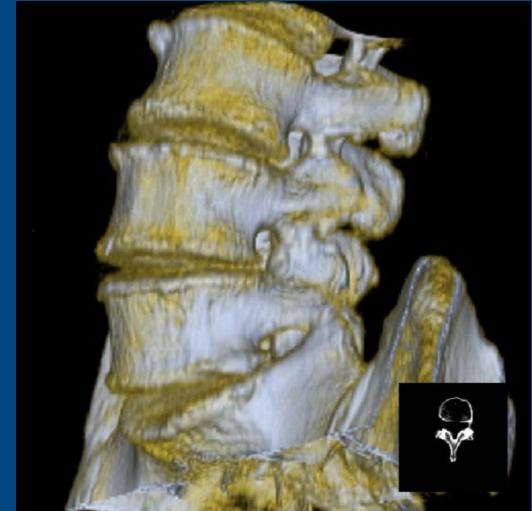
Knees



Extremities

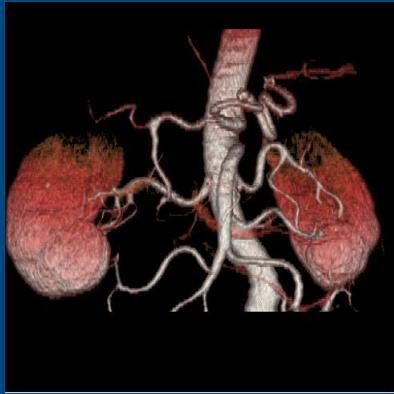


Spine

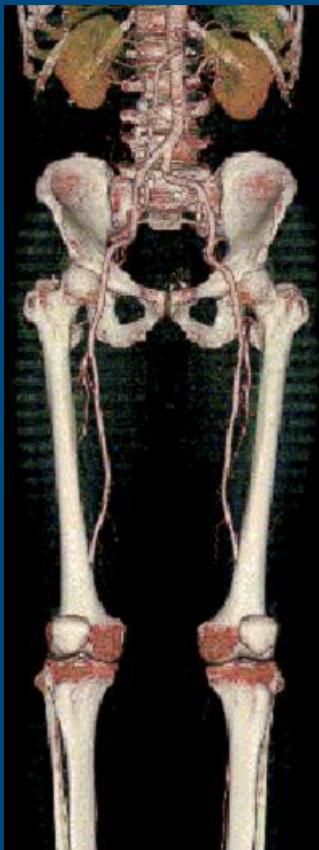


Clinical applications : angiography

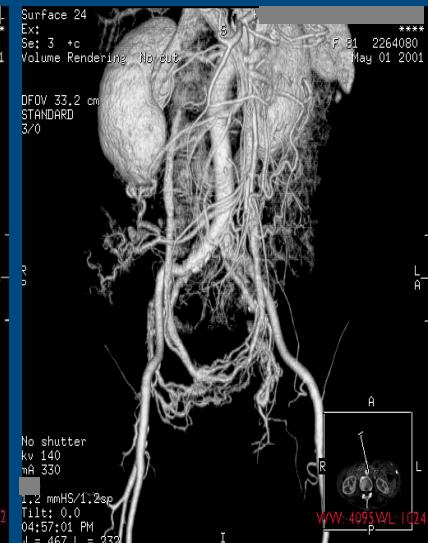
Renal agnio



Lower run offs



Abdominal aorta
Stent sizing



Carotids



MIP
image

Surface
rendering

The End