

Acquisition and Analysis of Biosignals

DTEK0042

Biosignal analysis III

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Introduction

So far, we learned:

- ❑ Time domain analysis and Frequency domain analysis
- ❑ Analysis of ECG, PPG, EMG, and PCG

In this session, we will learn:

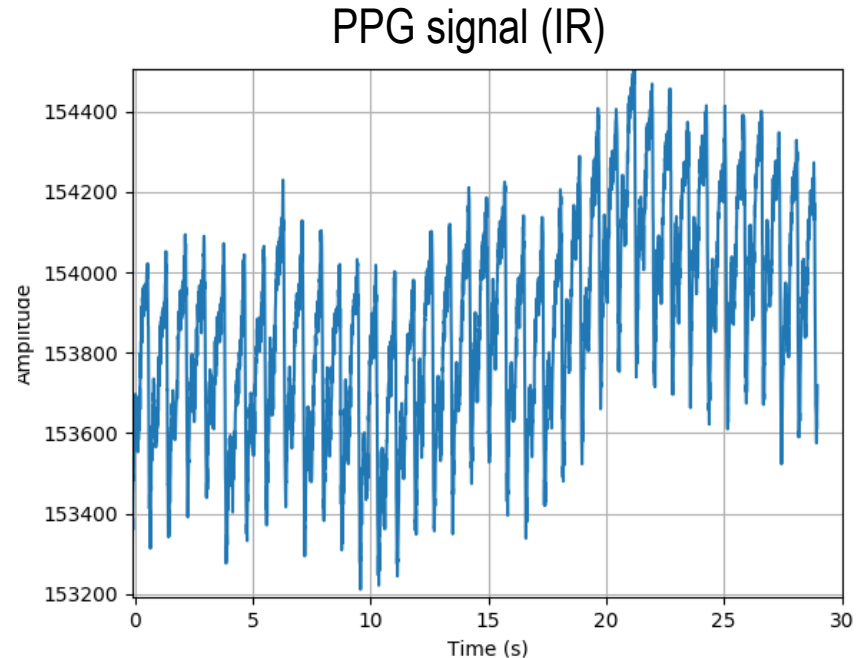
- ❑ Time-frequency analysis
- ❑ Analysis of SCG and GCG
- ❑ Classification and decision-making

Time domain analysis

❑ Different time-domain techniques are used to analyze the events

❑ Feature Extraction:

- Wave shape
- Intervals between events
- Energy distribution
- ...



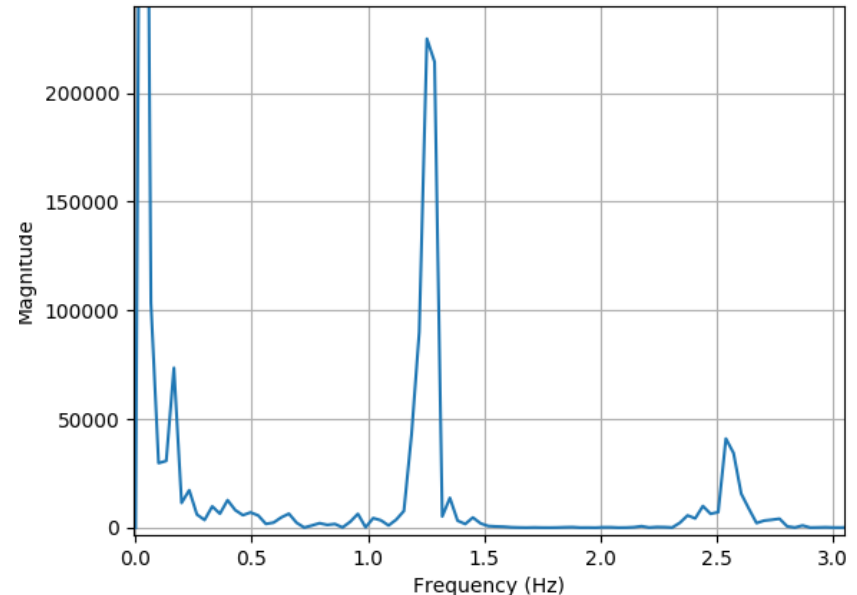
Frequency domain analysis

❑ Different frequency-domain techniques are used to analyze the events

❑ Feature Extraction:

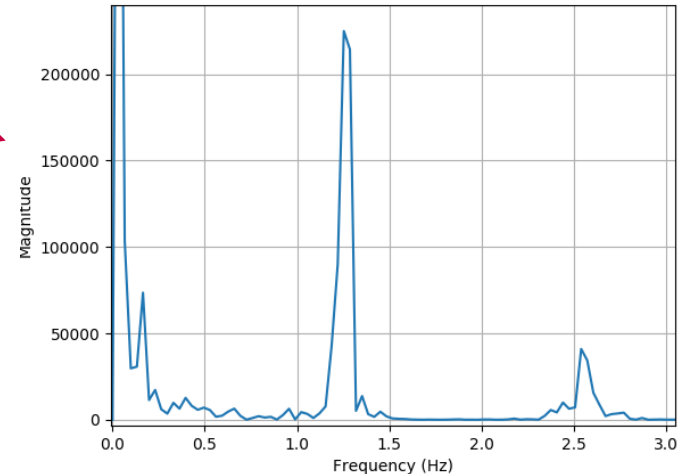
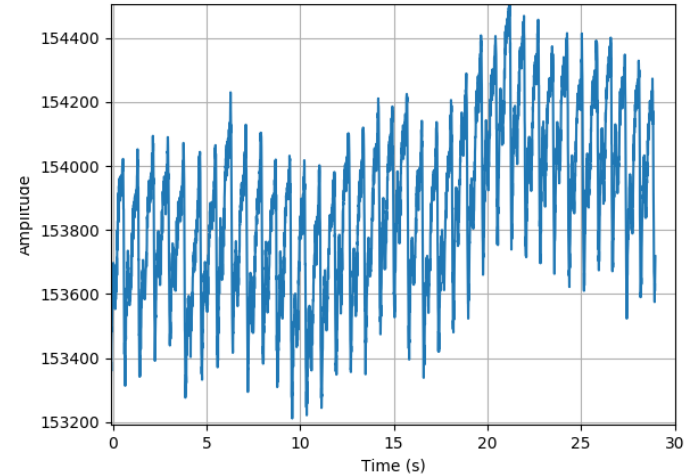
- Mean frequency
- Dominant frequency (resonance frequency)
- Power band
- ...

PSD of the PPG signal



Time domain analysis and Frequency domain analysis

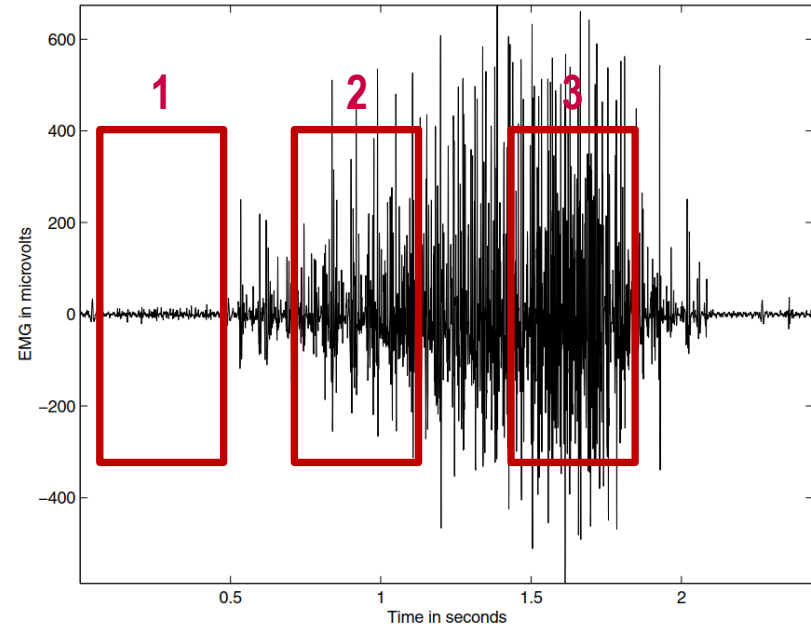
- ❑ **Time domain analysis:** We know when the event starts and when it ends, but it is difficult to understand the patterns, repetitive events, rhythms, etc.
- ❑ **Frequency domain analysis:** We know about the resonance frequency, but we do not know when the event starts and when it ends.
- ❑ How to use both the time and frequency information?



Time-Frequency Analysis

Nonstationary signals

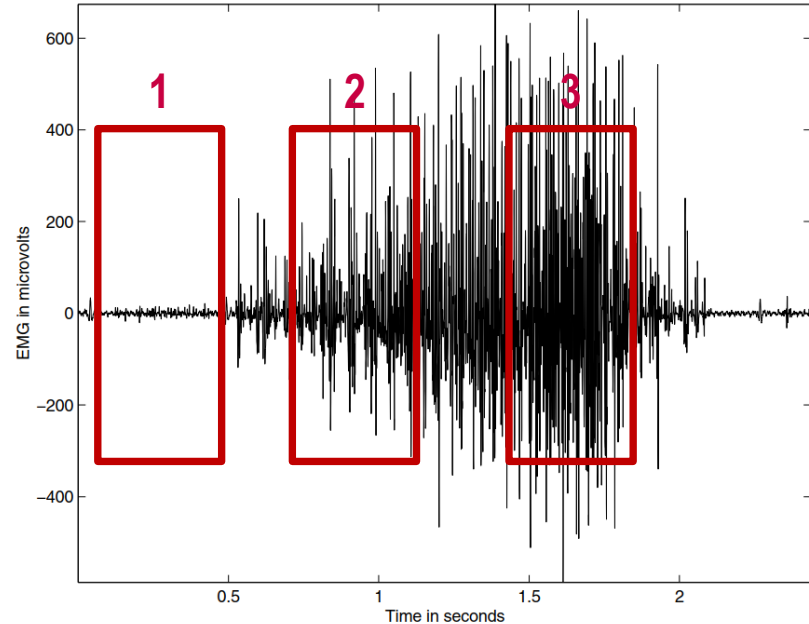
- ❑ A nonstationary signal possesses statistics that vary with time
- ❑ Various short-time statistical measures computed over moving windows may be used to characterize a nonstationary signal
 1. Mean
 2. Variance



Rangayyan, R. M. *Biomedical signal analysis*. 2nd Edition, Vol. 33. John Wiley & Sons, 2015.

Nonstationary signals – Cont.

3. Measures of activity
 - Nonstationary: turning points and zero crossing rate vary with time
4. Auto-correlation function (ACF) and power spectral density (PSD)
 - Nonstationary: ACF varies with time
 - If nonstationary in ACF, also nonstationary in its PSD



Rangayyan, R. M. *Biomedical signal analysis*. 2nd Edition, Vol. 33. John Wiley & Sons, 2015.

Fixed Segmentation

- ❑ Given a nonstationary signal, the simplest approach to break it into quasistationary segments would be to consider small windows of fixed duration.
- ❑ Let's consider the signal as $x(n)$ for $n = 0, 1, 2, \dots, N - 1$
- ❑ We could consider a fixed segment duration of M samples that $M \ll N$ and break the signal into $K = \frac{N}{M}$ parts as
$$x_k(n) = x[n + (k - 1)M]$$
$$0 \leq n \leq M - 1 \quad \text{and} \quad 1 \leq k \leq K$$
- ❑ With the assumption that the signal does not change its characteristics in the segment

Short time Fourier transform

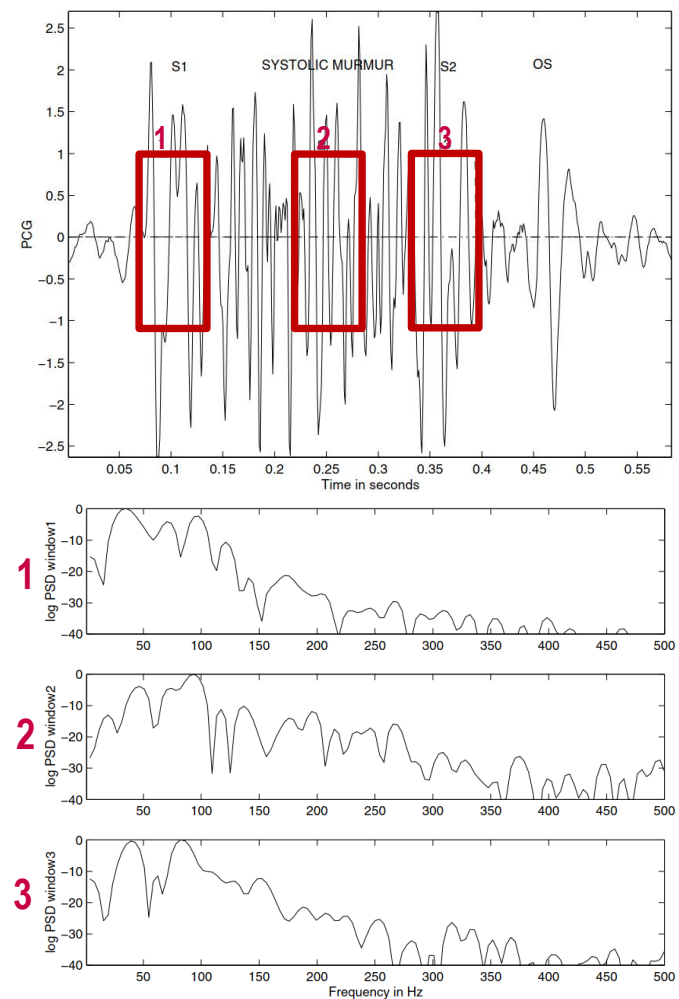
- ❑ Short time Fourier transform (STFT) is a sequence of Fourier transforms of a windowed signal
- ❑ For example:
 1. A given signal has been segmented into quasistationary parts $x_k(n)$
 2. We compute the DFT of each segment:

$$X_k(\omega) = \sum_{n=0}^{M-1} x_k(n) e^{-i\omega n}$$

- $X_k(\omega)$ for $k = 1, 2, \dots, K$ describe the time-varying spectral characteristics of the signal.

Example – PCG signal

- ❑ PCG signal (nonstationary) with systolic murmur and opening snap of the mitral valve
- ❑ The duration of each window is 64 samples, equal to 64ms with $f_s = 1 \text{ kHz}$
- ❑ The second window displaying the largest amount of high-frequency power due to the murmur



STFT – Moving analysis window

- ❑ Segmentation of the given signal may be interpreted as the application of a moving window to the signal where:

$$x_k(n) = x(n)w(n - m)$$

Any time instant



- ❑ We need to state how the window is moved from one segment to another.

STFT – Spectrogram

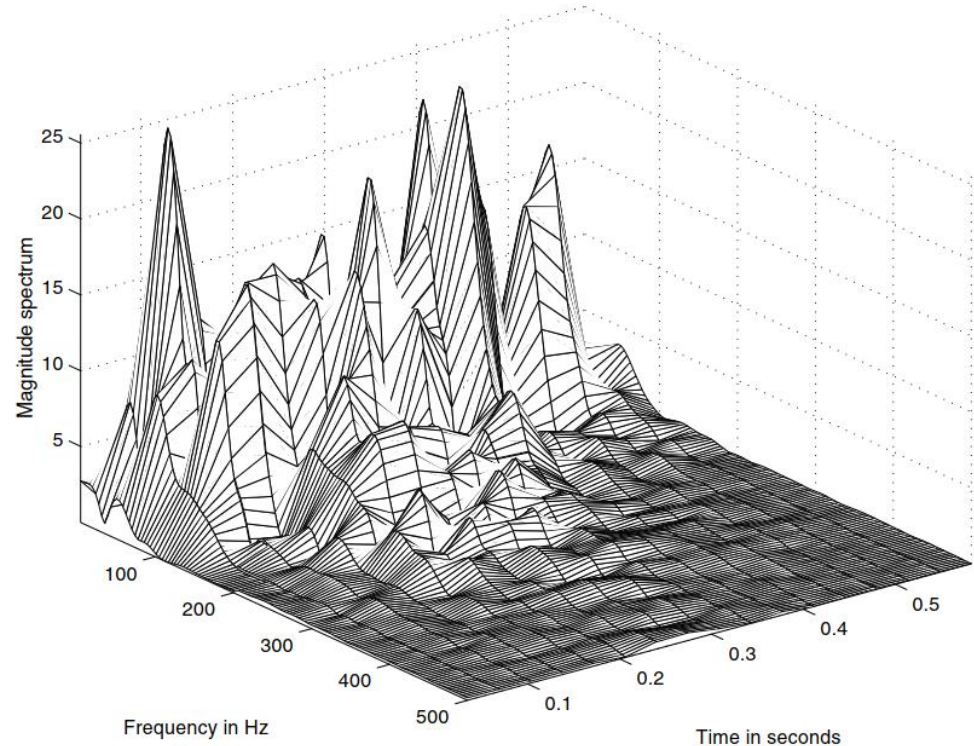
- We may then compute the Fourier transform of the segments:

$$X(m, \omega) = \sum_{n=0}^{M-1} [x(n)w(n - m)] e^{-i\omega n}$$

- The spectrum is now expressed
 - not only as a function of **frequency** ω ,
 - but also as a function of **time** m
- The magnitude of the STFT (squared) is known as the spectrogram of the signal.

Example – PCG signal

- ❑ PCG signal ($f_s = 1 \text{ kHz}$) with systolic murmur and opening snap of the mitral valve
- ❑ The duration of each window is 64 samples
- ❑ The window advance interval is 32 samples

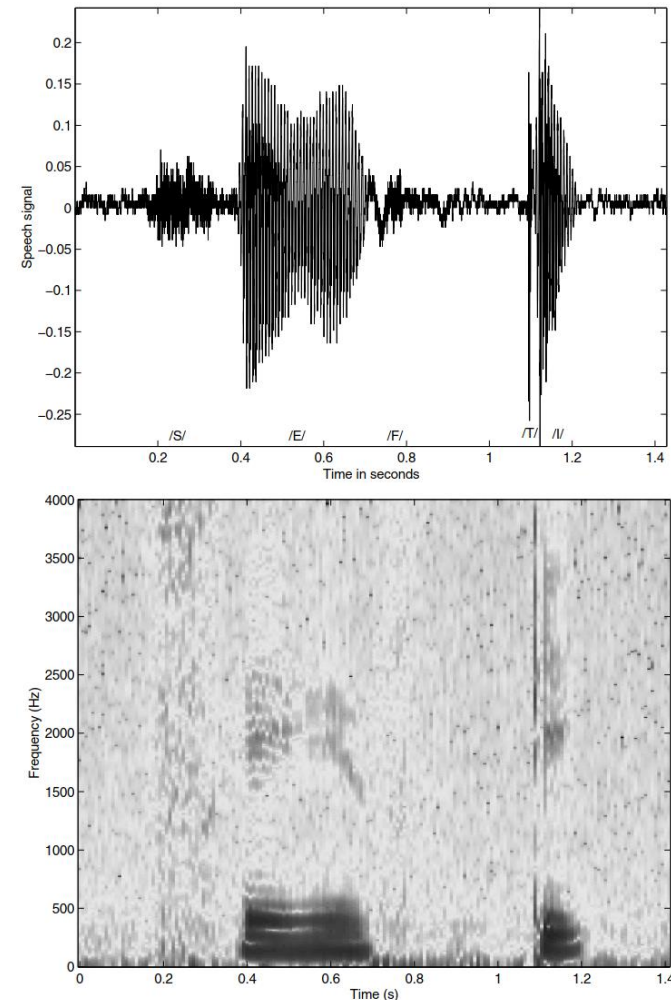


STFT – Analysis window

- ❑ We may advance the window (with size M):
 - M samples at a time: no overlap
 - One sample at a time: adjacent windows have an overlap of $(M - 1)$ samples.
 - $\frac{M}{2}$ samples at a time: an overlap of $\frac{M}{2}$ samples
- ❑ Some overlap is desirable in order to maintain continuity
- ❑ Duration of the segment (M): the window should be
 - Short enough to ensure that the segment is stationary
 - Long enough to permit meaningful analysis of low-frequency components
- ❑ We cannot simultaneously obtain arbitrarily high resolution along both the time and frequency axes

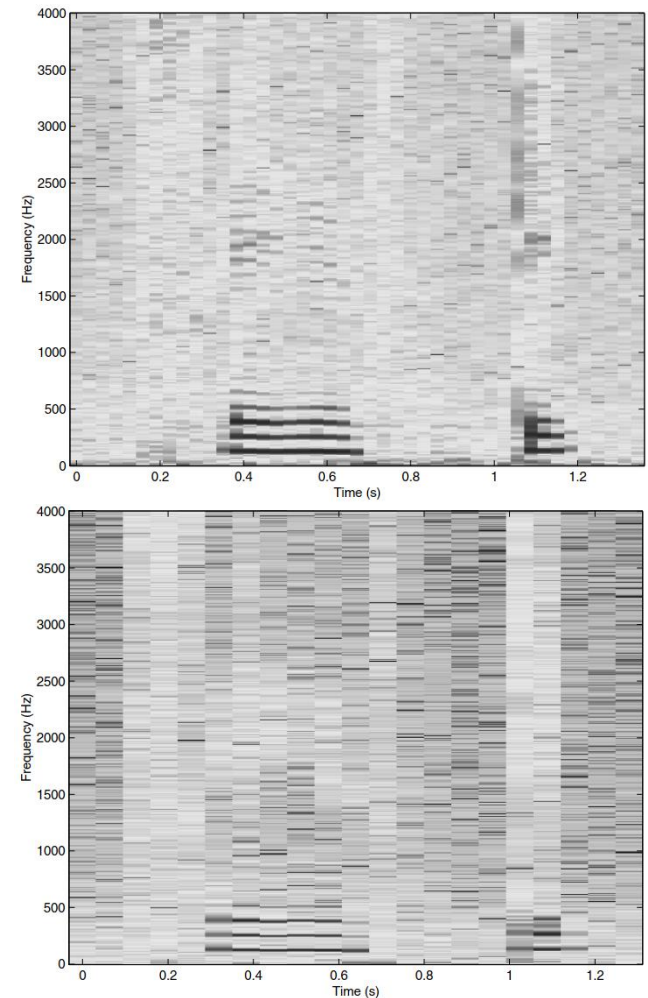
Example – Speech signal (1)

- ❑ The speech signal ($f_s = 8 \text{ kHz}$) of the word “Safety”
- ❑ In the spectrograms, the darkness at each point being proportional to the log PSD
- ❑ The analysis window duration is 16 ms (128 samples)
- ❑ The window advance interval is 8 ms
- ❑ The high-frequency nature of the fricatives is indicated (and plosive).



Example – Speech signal (2)

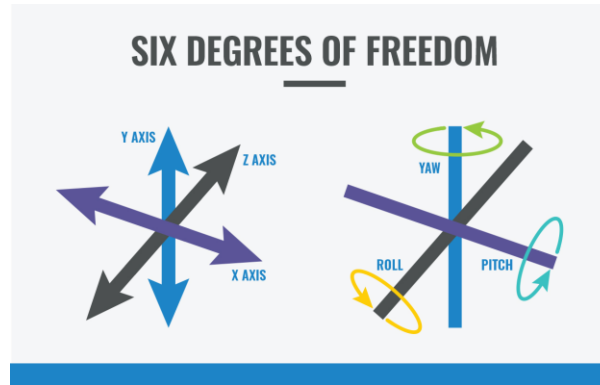
- ❑ In the upper figure:
 - The window duration is 64 ms (512 samples)
 - The window advance interval is 32 ms
- ❑ In the lower figure:
 - The window duration is 128 ms (1024 samples)
 - The window advance interval is 64 ms
- ❑ Increasing the length of the analysis window provides better frequency resolution while at the same time reducing the temporal resolution
- ❑ Decreasing the window length causes the reverse effects



Analysis of SCG and GCG

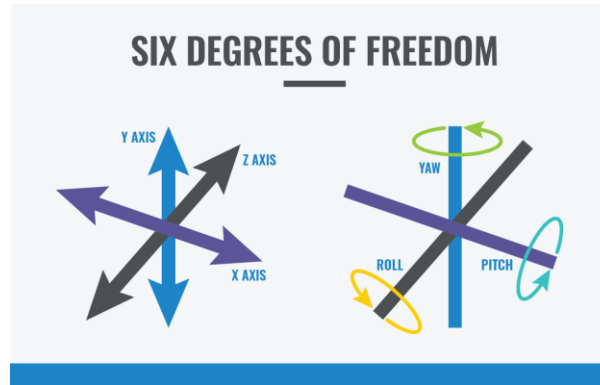
SCG and GCG

- ❑ Seismocardiography (SCG) is recorded by attaching an accelerometer to the chest approximately on top of the heart
- ❑ Gyrocardiography (GCG) is a similar technique for capturing rotational movement of the chest caused by the mechanical activity of the heart



SCG and GCG together

- Nowadays, we usually record both SCG and GCG signals. This results in a 6-dimensional signal value. In other words, 3 values for X, Y, and Z axis of acceleration and 3 values for X, Y, and Z axis of angular motion



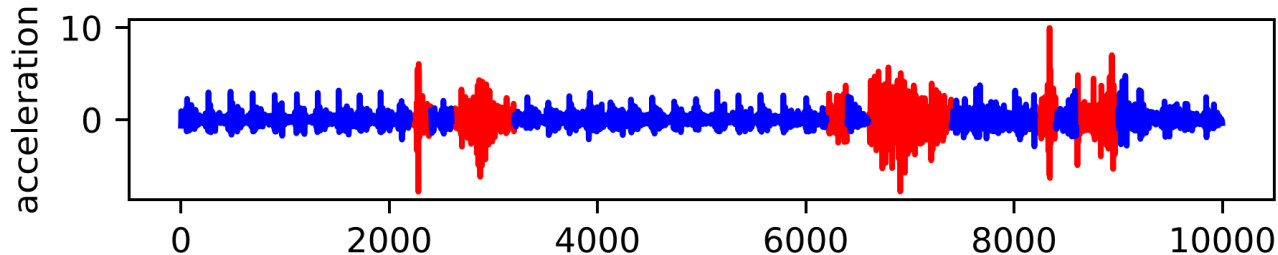
SCG and GCG preprocessing

❑ Baseline wander and noise removal

- filtering with Butterworth filter of order 4 and pass band 3-40 Hz

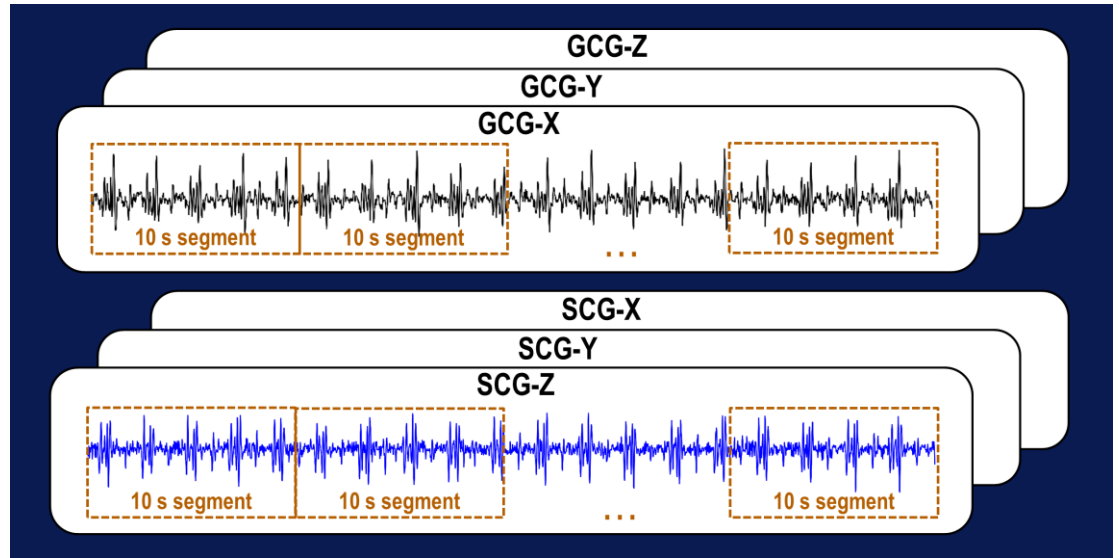
❑ Motion artifact rejection

- SCG is a motion tracking technique. If human body moves during SCG collection, there will be motion artefacts
 - Body movement and chest movements



Segmentation prior feature extraction

- Here we have SCG and GCG signals segmented by 10-second segments



Feature extraction (1)

❑ Time domain analysis

- Mean, standard deviation, median, interquartile range, entropy, zero crossing, cross-correlation, auto-correlation, mutual information, complexity, mobility, etc.

❑ Frequency domain analysis

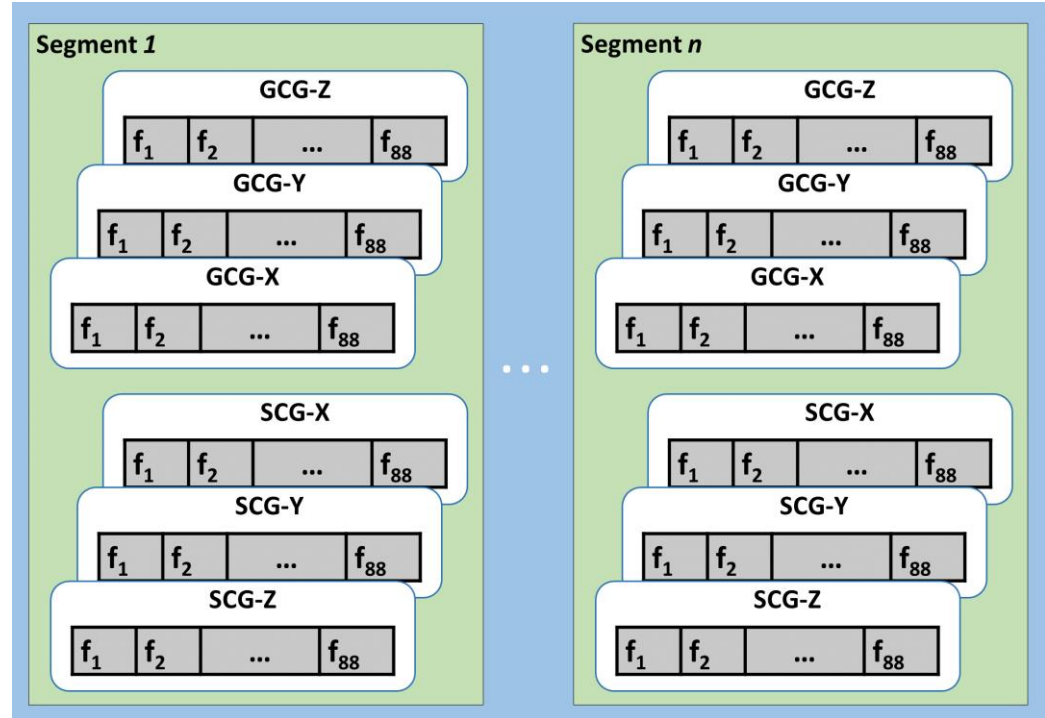
- Dominant frequency in Fourier domain, Fourier transform entropy, relative Fourier energy entropy, relative energy of each axis, etc.

❑ Time-frequency domain analysis

- Short Time Fourier Transform (STFT)

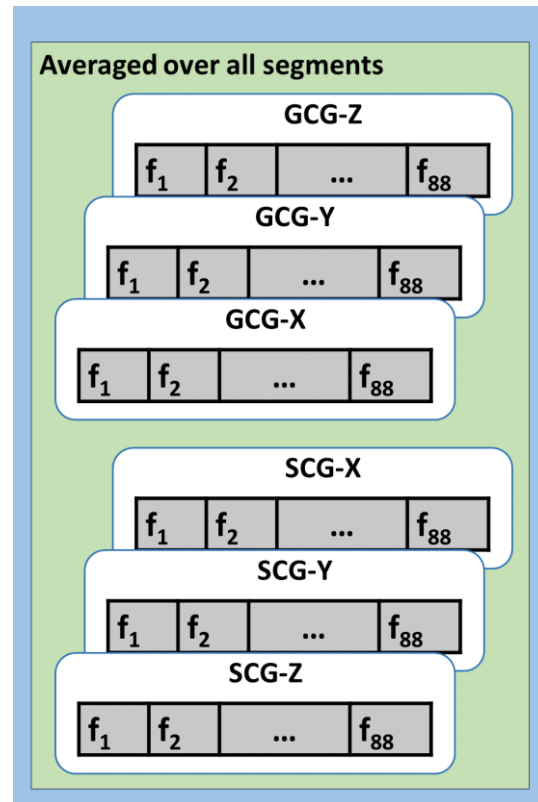
Feature extraction (2)

- For instance, 88 Features are extracted from each segment in each axis.



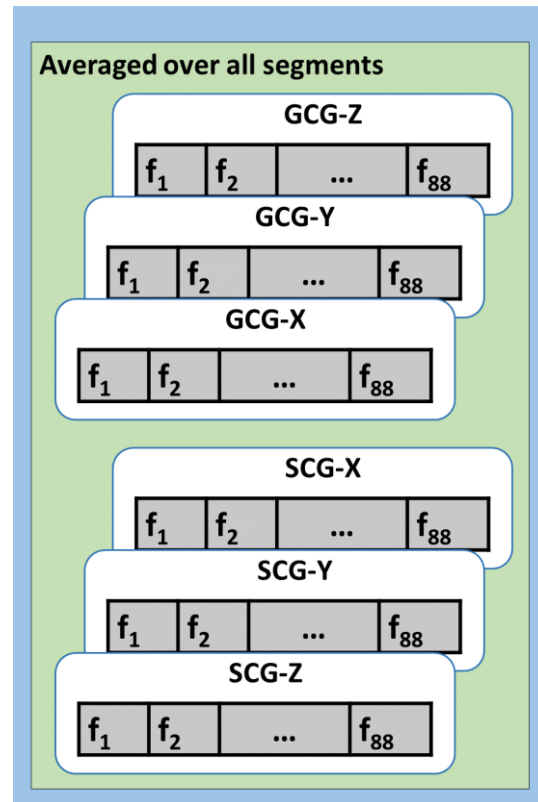
Averaging over all segments

- ❑ Averages will be calculated for each feature in each axis over the segments
- ❑ f_1 in GCG-Z is the average value of f_1 over all segments. This applies to all the other 5 axes.



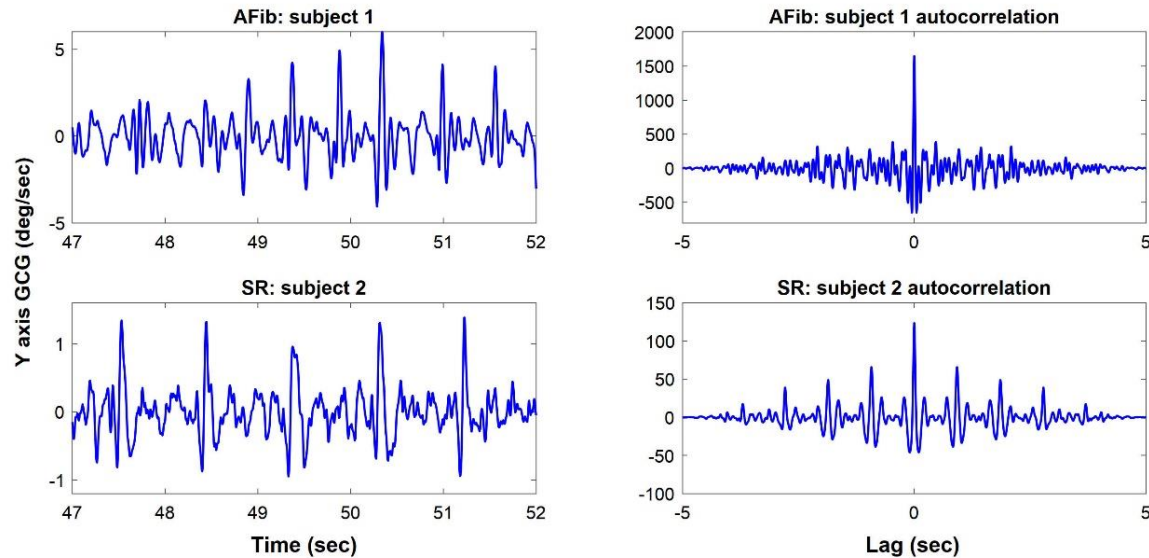
Why averaging?

- ❑ We need a robust view of a measurement
 - Random noise is removed
- ❑ In every measurement, we segment the signals into shorter episodes, extract features, and then average the features to get a robust view of every feature.

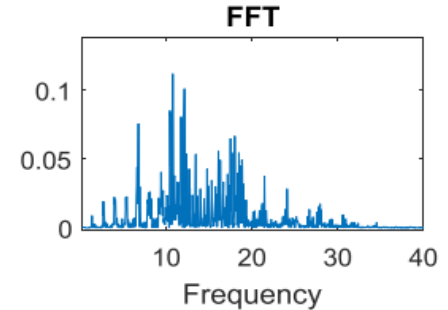
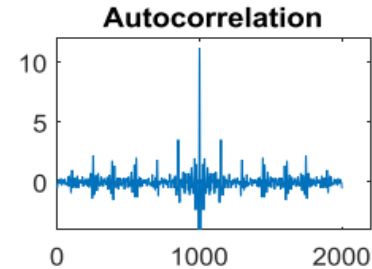
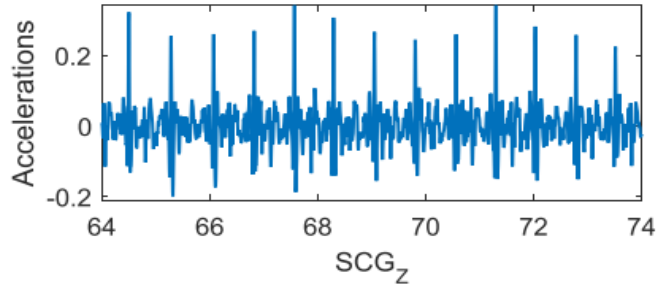
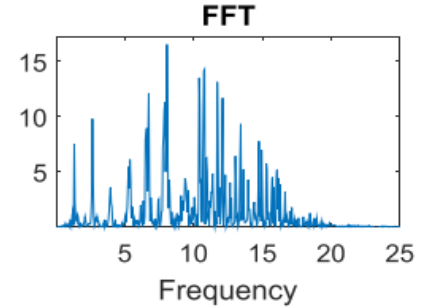
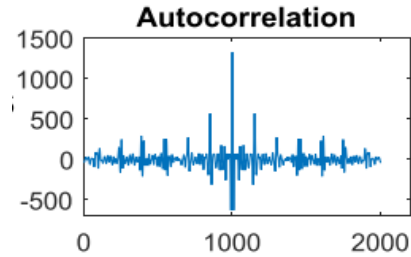
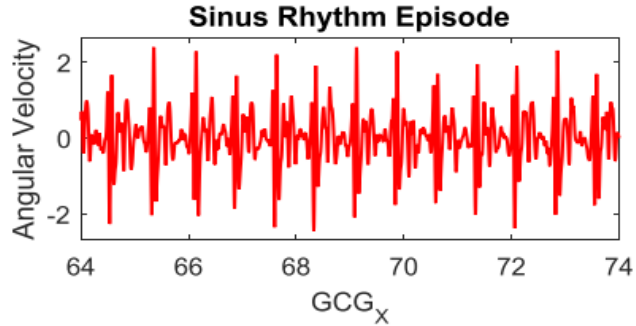


Autocorrelation (time domain)

❑ Auto-correlation for arrhythmia (atrial fibrillation) detection

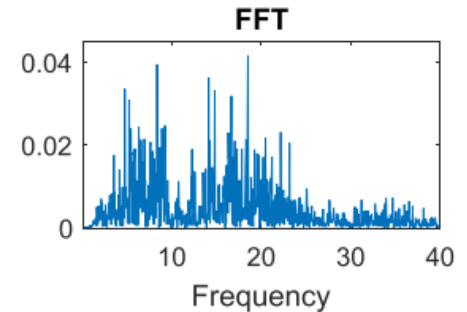
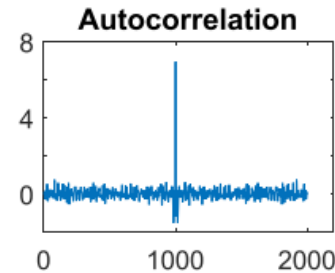
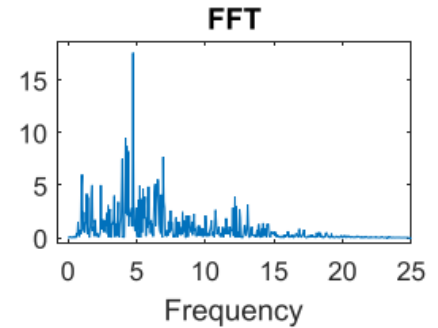
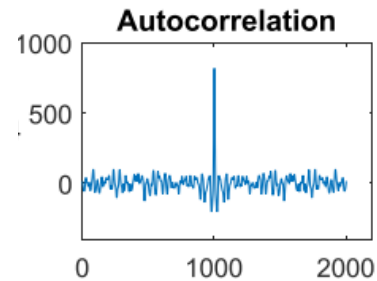
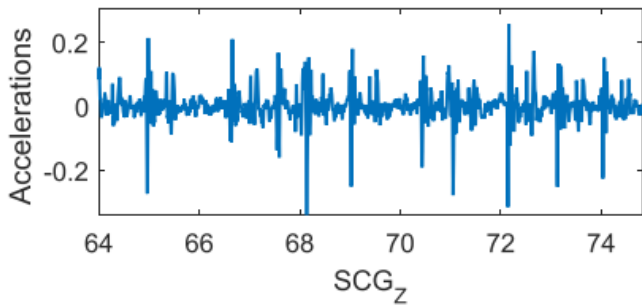
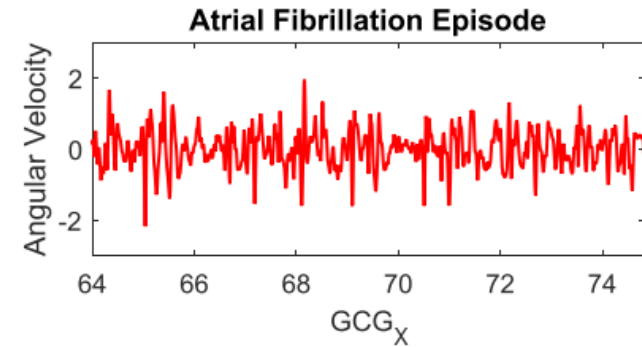


Autocorrelation and DFT – Normal



- Tadi, Mojtaba Jafari, et al. "Comprehensive Analysis of Cardiogenic Vibrations for Automated Detection of Atrial Fibrillation Using Smartphone Mechanocardiograms." *IEEE Sensors Journal* 19.6 (2018): 2230-2242.
- <https://www.dspguide.com/ch11/5.htm>

Autocorrelation and DFT – Atrial fibrillation

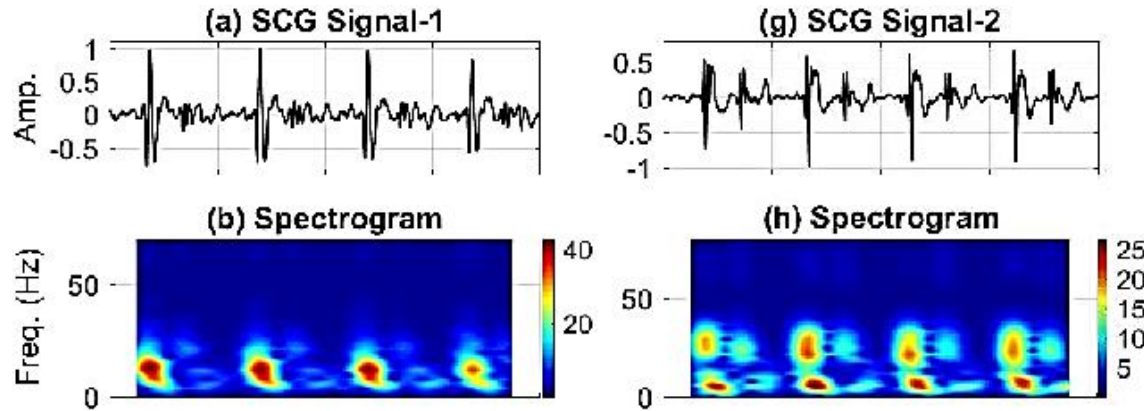


Frequency domain analysis

- ❑ **Dominant frequency:** the frequency that has the greatest magnitude in the Fourier domain.
 - Note that the DC frequency cannot be dominant frequency. We need to remove DC frequency before calculating dominant frequency.
 - Dominant frequency in sub-segments of a signal
 - Variations of dominant frequency among sub-segments: this parameter resembles heart rate variability but it is measured in frequency domain instead of time domain.

Time-frequency domain analysis

- **Spectrogram:** it helps us getting a view of time-frequency domain within a segment. Below are two short segments of SCG signals and their spectrograms.



Choudhary, Tilendra, L. N. Sharma, and M. K. Bhuyan. "Spectracentrogram: A Time-Frequency Distribution for Signal Processing Applications." 2018 International Conference on Intelligent Informatics and Biomedical Sciences (ICIIBMS). Vol. 3. IEEE, 2018.

Classification and Decision-making

Feature extraction

- ❑ Different features can be extracted from the biosignals:
 - ECG: RR interval, Duration of the ST segment, etc.
 - EMG: RMS value, turns count, etc.
 - SCG: mean, standard deviation, dominant frequency
- ❑ The features show the characteristics of the events
- ❑ The classification methods are utilized to categorize the events.
 - The inputs are the features
 - The output shows
 - if there is a disease or not
 - or the type of the disease

Rule-based methods

- ❑ The rule-based methods are any classification scheme that make use of IF-THEN rules for classification
- ❑ Rules can be set by experts or extracted from the data (depending on the application)
- ❑ There is a rule for each sample
- ❑ The data is classified using the rules

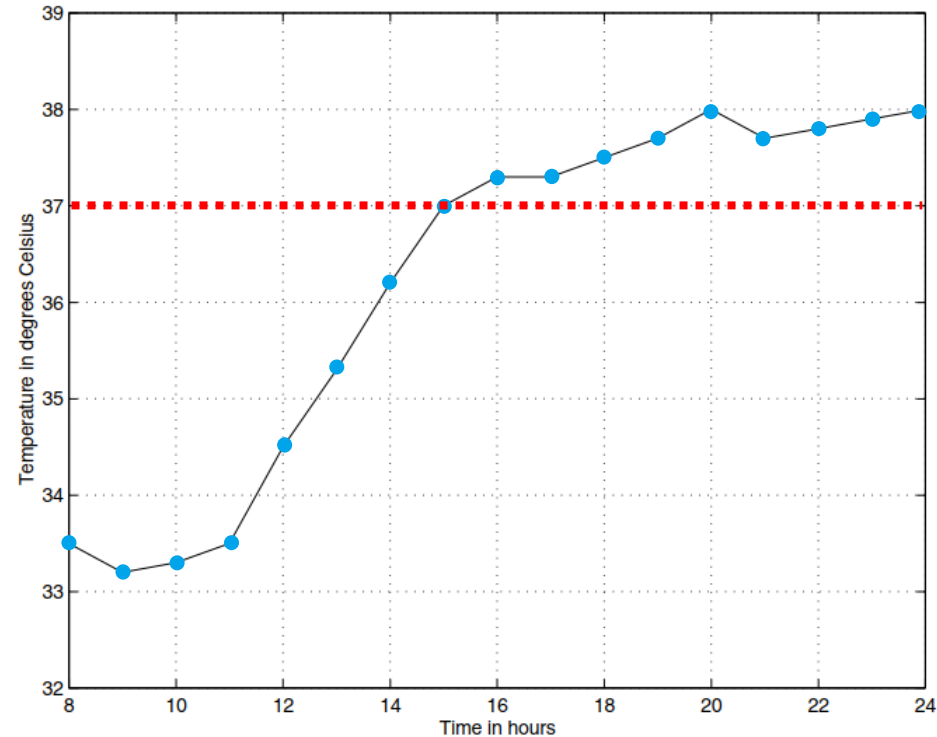
Example – simple threshold

Most infections cause a rise in the body temperature (BT)

Our measurement is discrete =>
 $x(n)$

$$x(n) = [x_1 \ x_2 \ x_3 \ \dots \ x_N]$$

E.g., to detect a disease: if the value of BT is higher than a **threshold** (e.g., 37°C)



Rangayyan, R. M. Biomedical signal analysis. 2nd Edition, Vol. 33. John Wiley & Sons, 2015.

Example – Early Warning Score

- ❑ Monitoring of vital signs allows early-detection of health deterioration.
- ❑ Early Warning Score (EWS) is a scoring method used in hospitals for assessment of patients' conditions.
- ❑ Higher scores are statistically linked to increased likelihood of health deterioration.

Physiological parameters	3	2	1	0	1	2	3
Respiration rate (breaths/minute)		0-8		9-14	15-20	21-29	30+
Oxygen saturation (%)	0%-84%	85%-89%	90%-94%	95%-100%			
Temperature (oC)		0-35		35.1-38.0		38.1-39.5	39.6+
Systolic BP (mmHg)	0-69	70-80	81-100	101-149	150-169	170-179	180+
Heart rate (beats/minute)	0-39	40-50	51-59	60-100	101-110	111-129	130+
Level of consciousness				A	V	P	U

* A=Alert, V=response to voice, P=response to pain, U=unresponsive

Example – Early Warning Score – Cont.

- ❑ Remote health monitoring systems includes sensors with limited resources (batteries)
- ❑ **From the system perspective:** A trade-off between energy-efficiency and measurement accuracy is needed
- ❑ A look-up table can be defined to reconfigure the system in a real-time fashion by observing the **EWS values**, **physical activity**, and **environmental situation**.
- ❑ More details can be found:
 - Anzanpour, A. et al., 2017, March. Self-awareness in remote health monitoring systems using wearable electronics. In Design, Automation & Test in Europe Conference & Exhibition (DATE), 2017 (pp. 1056-1061). IEEE.



Machine learning

- ❑ Machine learning techniques learn from examples data and past experience to perform specific tasks
 - E.g., categorize events into different classes
- ❑ Machine learning can extract models from the observation
 - Models can be defined as relationships between the variables (features) that describe the events.
- ❑ Trained models are used for the test data (to classify or predict)

Two references:

- Yaser S. Abu-Mostafa, Malik Magdon-Ismael, and Hsuan-Tien Lin. 2012. Learning from Data. AMLBook.
- Thomas Mitchell. 2012. Machine Learning. McGraw-Hill Education - Europe

Use in healthcare

☐ Abnormity (Disease) detection

- If the input data is normal vs abnormal
- Classify the diseases

☐ Body functions evaluation

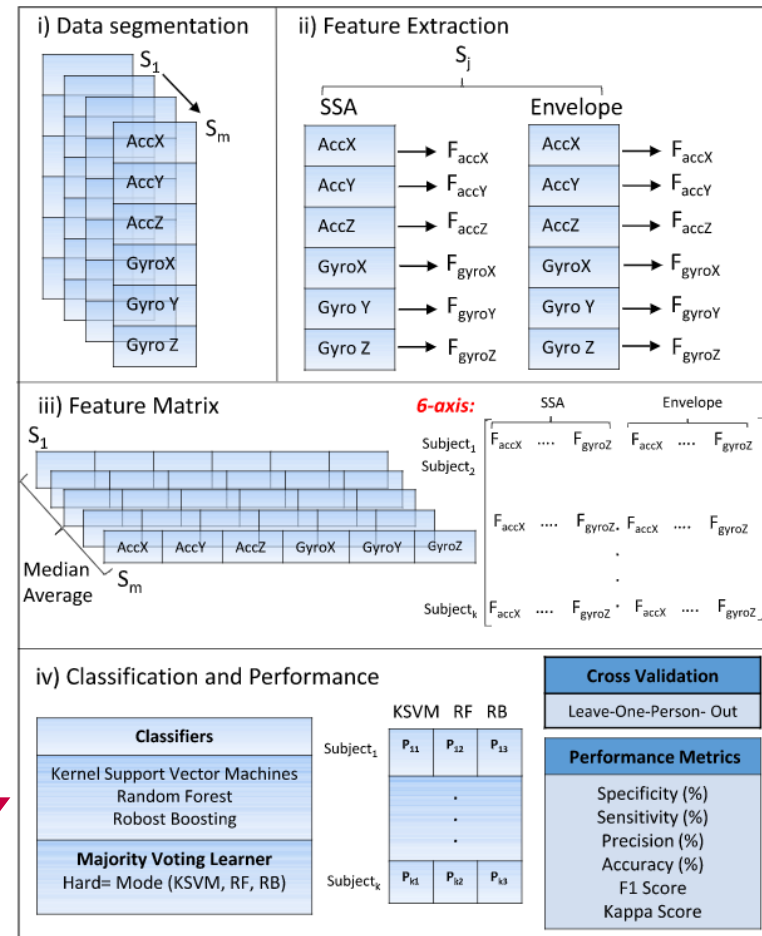
- E.g., neuromuscular system

☐ System optimization

☐ Others

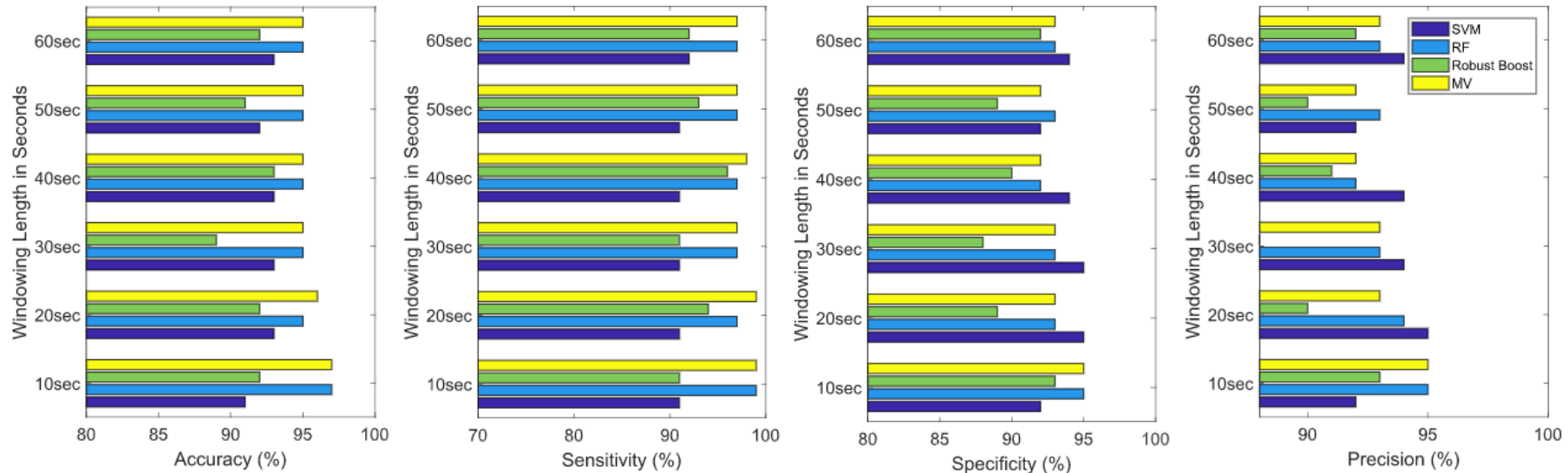
Example - Atrial fibrillation detection using SCG-GCG

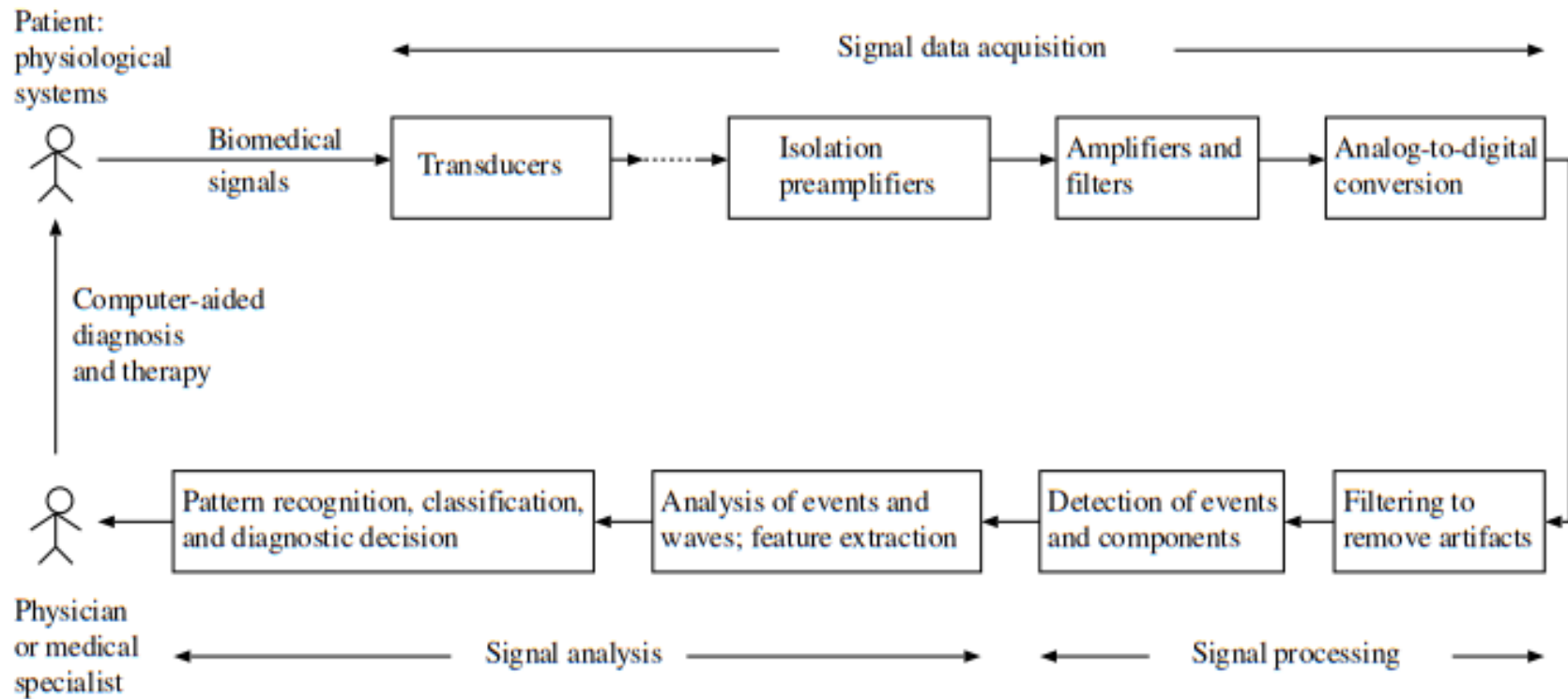
- ❑ Jafari Tadi, M. et al. "Comprehensive Analysis of Cardiogenic Vibrations for Automated Detection of Atrial Fibrillation Using Smartphone Mechanocardiograms." IEEE Sensors Journal 19.6 (2018): 2230-2242.
- ❑ Early diagnosis of AFib is a key step in the prevention of stroke and heart failure
- ❑ The SCG and GCG signals are collected from 435 users, including 190 AFib and 245 sinus rhythm cases, using a smartphone.
- ❑ The data analysis pipeline includes:



Example - Atrial fibrillation detection using SCG-GCG – Cont.

□ Classification performance in the cross-validation study with three classifiers and majority voting





Conclusion

In this session, we learned about:

- ☐ Time-frequency analysis
- ☐ Analysis of SCG and GCG
- ☐ Classification and decision-making

In the next lecture, we will have:

- ☐ A visiting lecturer from the Digital Health Technology group (UTU)
- ☐ Principal Component Analysis: a case study on finding respiration signal in high-dimensional sensor data

Thank You
Questions?



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