

# Multiscale Finite Volume Method

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# Outline

- 1 Standard Diffusion Equation
- 2 Example Diffusion terms
- 3 Finite Volume Solver
- 4 Simulation Results
- 5 Error Analysis
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## Diffusion Equation

- We solve the diffusion equation (1)

$$\nabla \cdot (D(x)\nabla c) = f(x) \quad \text{in } \Omega \quad (1)$$

$$c(x) = 0 \quad \text{on } \partial\Omega \quad (2)$$

- with Dirichlet boundary (2)
- We use constant source  $f(x) = 1, x \in \Omega$
- We use a Finite Volume solver

## Discretization

- Divide  $\Omega$  into a uniform grid  $\{Q_i\}$ 
  - cells  $Q_i$  are disjunct
  - $Q_i \cap Q_j = \emptyset, i \neq j$
  - we assume constant solution  $c_i$  on  $Q_i$
  - we assume constant source  $f(x) = f_i, x \in Q_i$

# Derivation of the 1D Finite Volume Method

## Integral Form

- since the Diffusion EQ.(1) holds on  $\Omega$ , it holds for any integral.
- $\implies$  (1) holds for the integral over  $Q_i$

$$\begin{aligned}\nabla \cdot (D(x)\nabla c) &= f(x) && \text{in } \Omega \\ \int_{Q_i} \nabla \cdot (D(x)\nabla c) &= \int_{Q_i} f(x) \, dx && i = 1, \dots, N\end{aligned}\tag{3}$$

- We use the constant source to evaluate the right hand side
- We transform (3) with the Stokes theorem
  - reduces the derivative degree on  $c$  and  $D$

$$\int_{\partial Q_i} D(x)\nabla c \cdot \vec{n} \, dS = |Q_i|f_i \quad i = 1, \dots, N\tag{4}$$

# Derivation of the 1D Finite Volume Method

## Numerical Flux

- constant solution
- $c$  is discontinuous on  $\partial Q$
- $\nabla c$  is not defined on the cell boundary
- we replace  $D(x)\nabla c$  with numerical flux  $\vec{g}$
- $\vec{g}$  describes flux of the solution between neighbouring cells

$$\int_{\partial Q_i} D(x) \nabla c \cdot \vec{n} \, dS = \int_{Q_i} f(x) \, dx \quad i = 1, \dots, N \quad (5)$$

$$\int_{\partial Q_i} \vec{g}(c^+, c^-) \cdot \vec{n} \, dS = \int_{Q_i} f(x) \, dx \quad i = 1, \dots, N \quad (6)$$

## 1D Flux

We employ the flux approximation introduced in the MMM Lecture. Since we only investigated diffusion terms with an analytical representation, we are able to calculate this value directly.

$$g(c^+, c^-) = -D(x^{\frac{1}{2}+}) \frac{c^+ - c^-}{h} \quad (7)$$

Furthermore, we introduce transmissivities  $T_{\pm}$  between both cells.

$$g(c^+, c^-) = T_{\pm} * (c^+ - c^-)$$
$$T_{\pm} = -D(x^{\frac{1}{2}+}) \frac{1}{h}$$



# Numerical flux approximation

## 2D Flux

We define the flux term  $\vec{g} := (g_x, g_y)^T$  in 2 Dimensions very similar to those in one dimension.

$$g_x(c_{i+1,j}, c_{ij}) = -\Delta_y D(x_{i+\frac{1}{2},j}) \frac{c_{i+1,j} - c_{ij}}{\Delta_x} \quad (8)$$

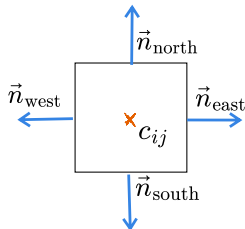
$$g_y(c_{i,j+1}, c_{ij}) = -\Delta_x D(x_{i,j+\frac{1}{2}}) \frac{c_{i,j+1} - c_{ij}}{\Delta_y} \quad (9)$$

and in the same manner we introduce 2D transmissions  $T_{i+1j}^x, T_{ij+1}^y$

$$g_x(c_{i+1j}, c_{ij}) = T_{i+1j}^x (c_{i+1j} - c_{ij})$$

$$g_y(c_{ij+1}, c_{ij}) = T_{ij+1}^y (c_{i+1j} - c_{ij})$$

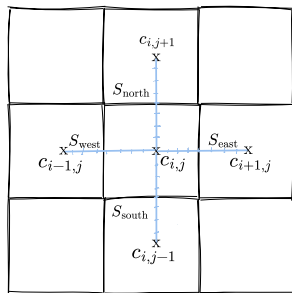
Reference Cell for finite Volume



- only 4 normals in 2D (2 in 1D)
- integral simplifies

$$\int_{\partial Q_i} \vec{g}(c^+, c^-) \cdot \vec{n} \, dS = |Q_i| f_i$$
$$\sum_{n \in \partial Q} \vec{g}(c_{ij+\vec{n}}, c_{ij}) \cdot \vec{n} = |Q_i| f_i$$

2D Macro / 1D Micro FV



- Adds microscale simulation
  - one dimensional
  - for each normal
  - $n$  subgrid cells
- Calculates Transmissions  $T_S$ 
  - with microscale solution  $\phi_S$

$$T_S = - \int_{S_0}^{S_1} D(x) (\phi'_S(\vec{x}))^2 dS$$

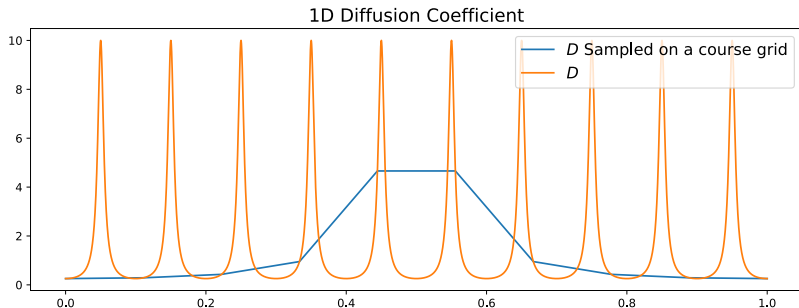
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Since the aim of multiscale Finite Volume is to improve the results for highly fluctuating diffusivities.

## Code

```
def oscillation(x, eps = 0.1):  
    return 1 / (2+1.9 * np.cos(2 * np.pi* x / eps))
```

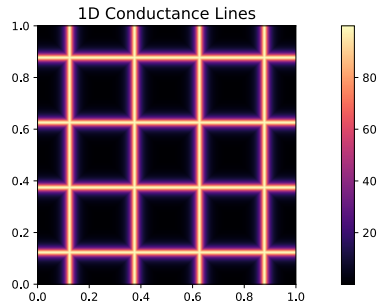
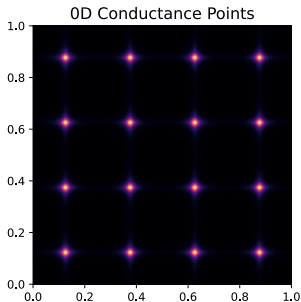


# 2D Oscillation

## Code

```
def osc2D_point(x,y , eps = 0.25):  
    return oscillation(x, eps=eps) * oscillation(y, eps=eps)  
def osc2D_line(x,y , eps = 0.25):  
    return np.maximum(oscillation(x, eps=eps) , oscillation(y,  
        ↪ eps=eps))
```

Oscillating Diffusion



# 2D Box Condition

To test numerical stability of our methods, we introduce a box constraint that traps some concentration in the center.

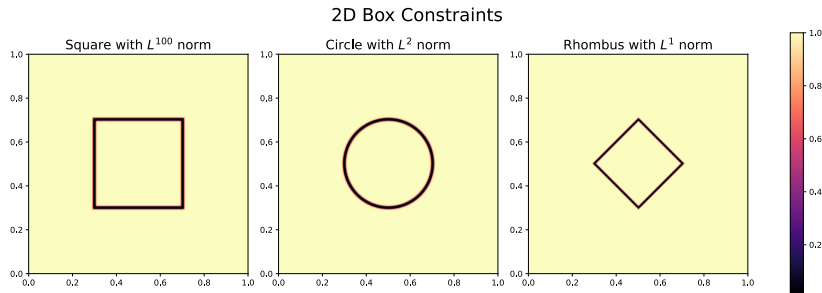


Figure: Constraints restricting flow from the center of the Domain

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# Program Structure

## Class Structure

```
class FVSolver:
    N : int
    resolution : int
    h : np.float64
    x : NDArray[np.float64]
    D : Callable
    f : NDArray[np.float64]
    c : NDArray[np.float64]
    micro_basis : NDArray[np.float64]
    _T : NDArray[np.float64]

<<Init>>
<<Assemble Matrix>>
<<Boundary>>
<<Solve>>
<<Microscale Transmissions>>
<<Reconstruct Microscale Solution>>
```

## Initialization

```
def __init__(self , N :int , D :Callable , domain=(0.,1.))->None:
    self.h = (domain[1] - domain[0]) / (N-1)
    self.N = N
    self.D = D
    self.x = np.linspace(domain[0] , domain[1] , N)
    self._T = -1/self.h * D((self.x[:-1] + self.x[1:])*0.5)
    self.f = self.h* np.ones(N)
```

## Boundary

```
def set_boundary(self , bc=(0.,0.)):  
    self.f[0] = bc[0]  
    self.f[-1] = bc[1]
```

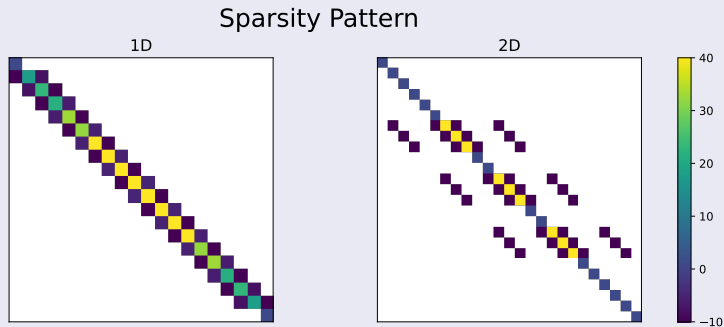
## Solving

```
def solve(self):  
    self.c = spsolve(self._A.tocsr() , self.f)  
    return self.c
```

## Matrix Assembly

```
def assemble_matrix(self)-> None:
    diagp1 = np.zeros(self.N)
    diagp1[2:] = self._T[1:]
    diagm1 = np.zeros(self.N)
    diagm1[:-2] = self._T[:-1]
    diag0 = np.ones(self.N)
    diag0[1:-1] = -1 * (self._T[1:] + self._T[:-1])
    self._A = spdiags([diagm1 , diag0 , diagp1] , np.array( [-1, 0,
↪ 1] ))
```

## Sparsity Pattern of the linear system

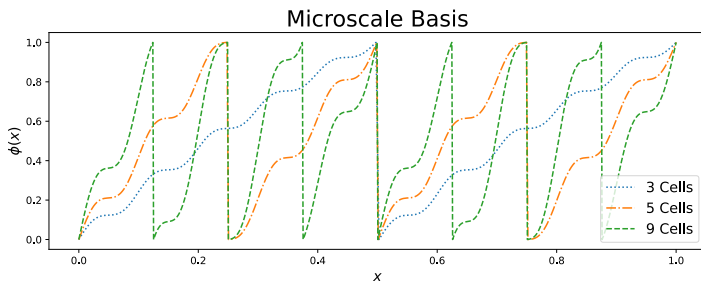
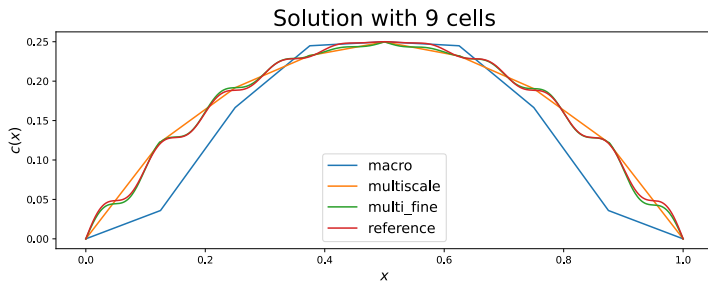


**Figure:** Non zeros values of the system matrices for a 20 cell 1D and a  $5 \times 5$  cell 2D system.

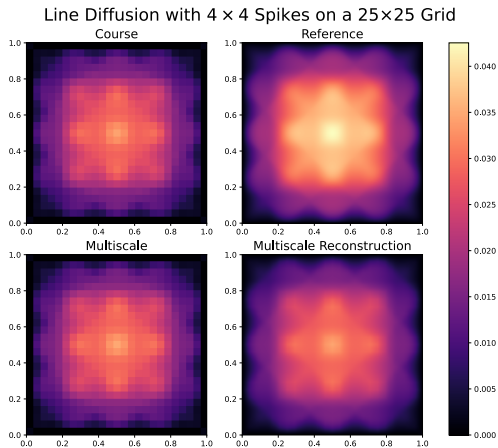
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# 1D Oscillating Diffusion



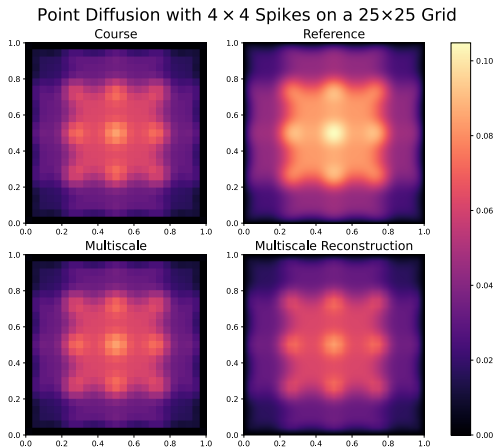
# Line Diffusion



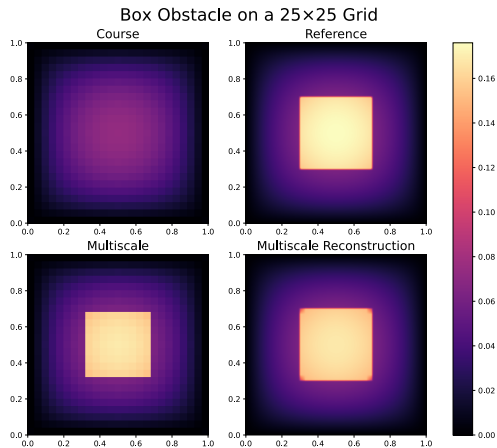
**Figure:** Comparison of different 2D solutions with a  $1000 \times 1000$  reference solution.



# Point Diffusion

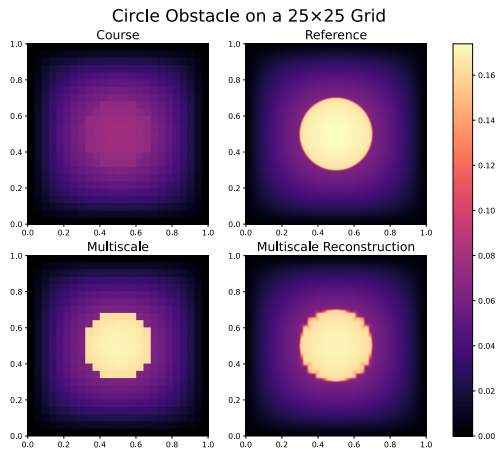


**Figure:** Comparison of different 2D solutions with a  $1000 \times 1000$  reference solution.



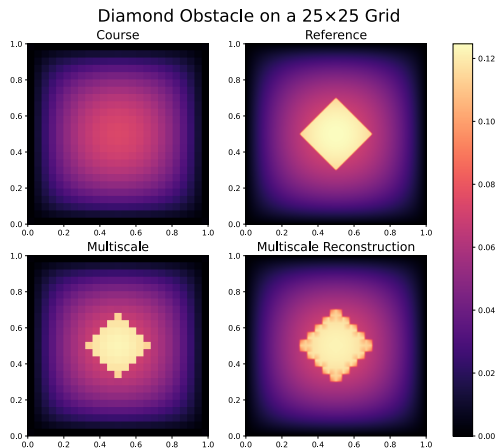
**Figure:** Comparison of different 2D solutions with a  $1000 \times 1000$  reference solution.

# 2D Circle



**Figure:** Comparison of different 2D solutions with a  $1000 \times 1000$  reference solution.

# 2D Diamond

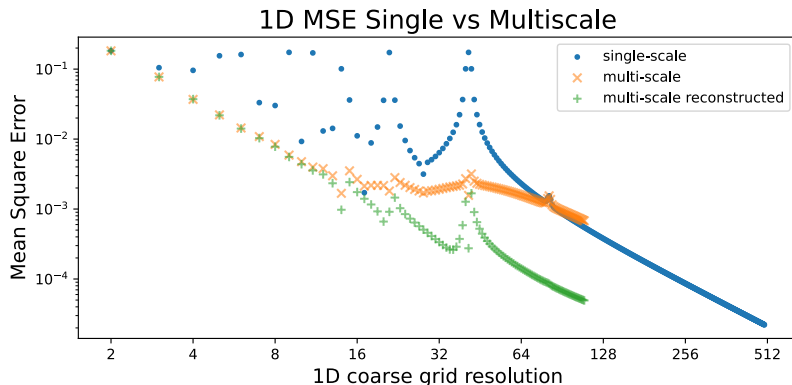


**Figure:** Comparison of different 2D solutions with a  $1000 \times 1000$  reference solution.

# Outline

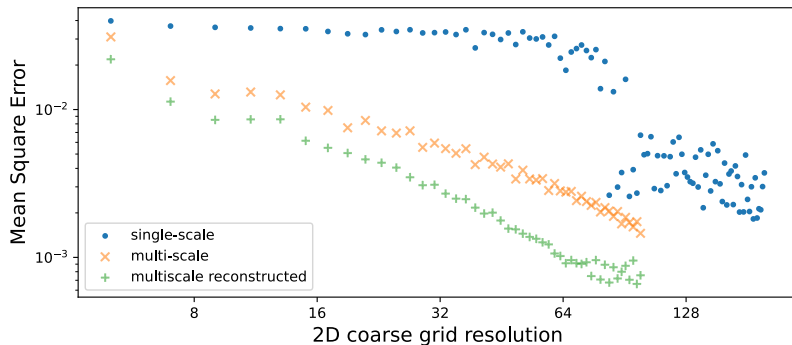
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# 1D Oscillating Diffusion



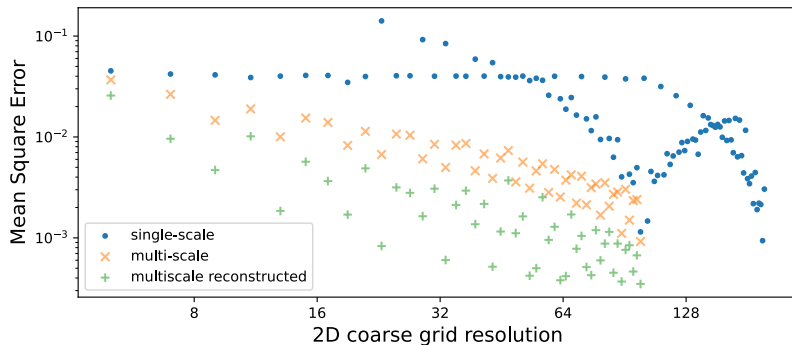
**Figure:** Mean Square Error (MSE) against a reference solution with a 1000 cell reference grid. For a 1D diffusion with 20 spikes and a 1000 cell microscale resolution.

## 2D MSE Single vs Multiscale



**Figure:** Mean Square Error (MSE) against a reference solution with a  $1000 \times 1000$  cell reference grid. For a circular Obstacle and a 100 cell microscale resolution.

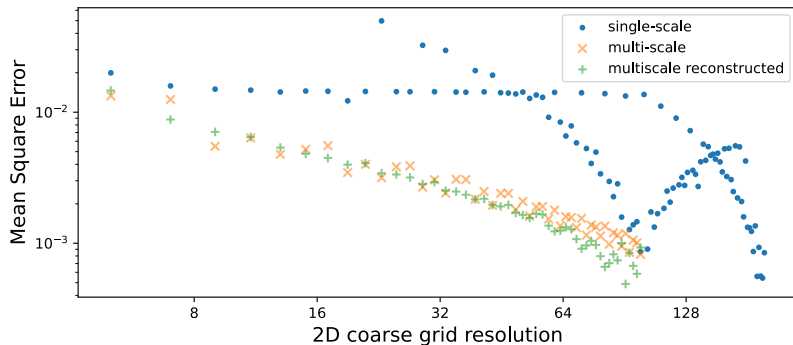
## 2D MSE Single vs Multiscale



**Figure:** Mean Square Error (MSE) against a reference solution with a  $1000 \times 1000$  cell reference grid. For a box Obstacle and a 100 cell microscale resolution.

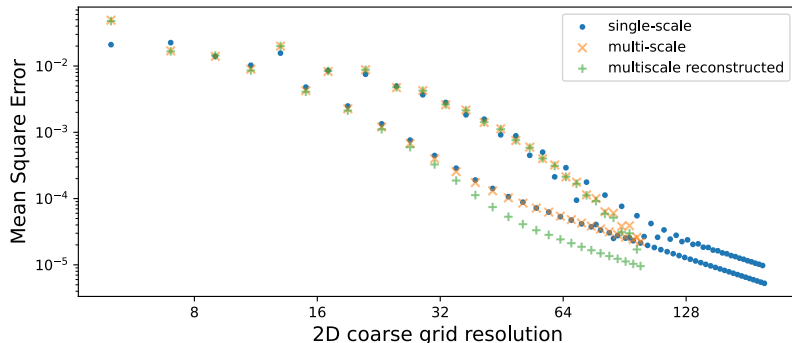


## 2D MSE Single vs Multiscale



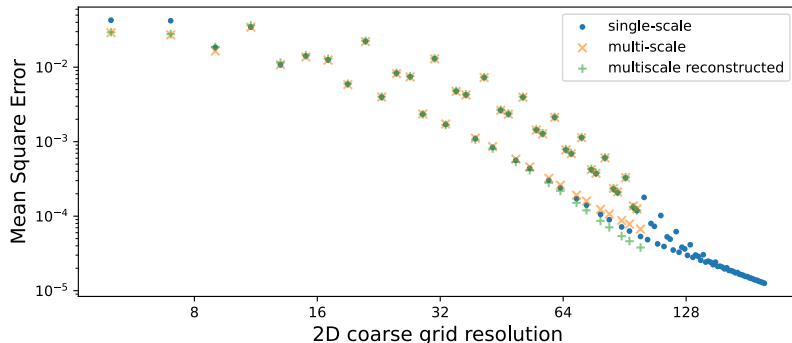
**Figure:** Mean Square Error (MSE) against a reference solution with a  $1000 \times 1000$  cell reference grid. For a diamond obstacle and a 100 cell microscale resolution.

## 2D MSE Single vs Multiscale



**Figure:** Mean Square Error (MSE) against a reference solution with a  $1000 \times 1000$  cell reference grid. For a line diffusion with 4 spikes and a 100 cell microscale resolution.

## 2D MSE Single vs Multiscale



**Figure:** Mean Square Error (MSE) against a reference solution with a  $1000 \times 1000$  cell reference grid. For a point diffusion with 4 spikes and a 100 cell microscale resolution.

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- works well for 1D
  - no performance benefit
  - expensive microscale simulations
  - worse if single scale can resolve the details
  - reconstruction works very well
- works well for some 2D cases
  - can resolve thin walls
  - can reconstruct only orthogonal detail
- no benefit in other cases
  - no benefit for point and line diffusion
- requires some differentiability conditions on  $D(\vec{x})$

# Further Considerations

- multipoint flux approximation
- higher order 2D reconstruction
- realistic diffusion with interpolated high res data
- 3D
- irregular grid
- parallelization to make use of independent microscale simulations