

SPECTPSFToolbox: A Python Toolbox for SPECT Point Spread Function Modeling

Luke Polson^{1,2*}, Carlos Uribe^{2,4,5*}¶, and Arman Rahmim^{1,2,3,5¶}

¹ Department of Physics & Astronomy, University of British Columbia, Vancouver Canada ² Department of Integrative Oncology, BC Cancer Research Institute, Vancouver Canada ³ School of Biomedical Engineering, University of British Columbia, Vancouver Canada ⁴ Department of Radiology, University of British Columbia, Vancouver Canada ⁵ Molecular Imaging and Therapy Department, BC Cancer, Vancouver Canada ¶ Corresponding author * These authors contributed equally.

DOI: [10.xxxxxx/draft](https://doi.org/10.xxxxxx/draft)

Software

- [Review](#) ↗
- [Repository](#) ↗
- [Archive](#) ↗

Editor: [Open Journals](#) ↗

Reviewers:

- [@openjournals](#)

Submitted: 01 January 1970

Published: unpublished

License

Authors of papers retain copyright and release the work under a Creative Commons Attribution 4.0 International License ([CC BY 4.0](#)).

In partnership with



AMERICAN
ASTRONOMICAL
SOCIETY

This article and software are linked with research article DOI [10.3847/xxxxx](https://doi.org/10.3847/xxxxx) <- [update this with the DOI from AAS once you know it.](#), published in the *Astrophysical Journal* <- The name of the AAS journal..

Summary

SPECTPSFToolbox is a python toolbox for SPECT point spread function (PSF) fitting. The library provides functionality for obtaining comprehensive PSF models that can be used in the python library PyTomography ([Polson et al., 2024](#)) for SPECT reconstruction. The models are constructed from linear operators that can be chained together and fit to Monte Carlo (MC) or real point source data.

Statement of need

SPECT imaging is used to measure the 3D distribution of a radioactive molecule within a patient; it requires (i) acquisition of 2D projection images at different angles using a gamma camera followed by (ii) use of a tomographic image reconstruction algorithm to obtain a 3D radioactivity distribution consistent with the acquired data ([Barrett et al., 2003](#)). The gamma cameras used in SPECT imaging have finite resolution: infinitesimal point sources of radioactivity show up as finite “point spread functions” (PSF) on the camera. The PSF consists of three main components: (i) the geometric component (GC) which depends on the shape and spacing of the collimator bores, (ii) the septal penetration component (SPC) which results from photons that travel through the collimator material without being attenuated, and (iii) the septal scatter component (SSC), which consists of photons that scatter within the collimator material and subsequently get detected in the scintillator. When the thickness of the SPECT collimator sufficiently matches the energy of the detected radiation, the PSF is dominated by the GC and can be sufficiently approximated using a distance dependent Gaussian function. When the energy of the photons is large relative to the thickness and hole size of the collimator material, the PSF contains significant contributions from SPC and SSC and it can no longer be approximated using simple Gaussian functions.

Unfortunately, many currently available open source reconstruction library only provide support for Gaussian PSF modeling which can only capture the GC. Given the recent success of ²²⁵Ac based radiopharmaceuticals for prostate cancer treatment that emit high energy photons ([Delker et al., 2023](#); [Kratochwil & others, 2018](#); [Liubchenko & others, 2024](#); [Rosar & others, 2021](#); [Sathekge & others, 2020](#); [Zacherl & others, 2021](#)), there is a need for tools that provides comprehensive SPECT PSF modeling that include SPC and SSC. This python based library provides the tools to build general SPECT PSF models. The developed models can be saved and used in open source image reconstruction libraries, such as PyTomography.

Overview of SPECTPSFToolbox

The purpose of SPECT reconstruction is to estimate the 3D radionuclide concentration f that produces the acquired detector data g given an analytical model for the imaging system, known as the system matrix. Under standard conditions, the SPECT system matrix estimates the projection g_θ at angle θ as

$$g_\theta(x, y) = \sum_d \text{PSF}(d) [f'(x, y, d)] \quad (1)$$

where (x, y) is the position on the detector, d is the perpendicular distance to the detector, f' is the attenuation adjusted image corresponding to the detector angle, and $\text{PSF}(d)$ is a 2D linear operator that operates separately on f at each distance d . The toolbox provides the necessary tools to obtain $\text{PSF}(d)$.

The toolbox is separated into three main classes

1. 'Kernel1D': objects that take in 1D position x , source-detector distance d , hyperparameters b , and return a 1D kernel at each source-detector distance.
2. 'Kernel2D': objects that take in a 2D meshgrid (x, y) , source-detector distance d , hyperparameters b , and return a 2D kernel at each source-detector distance.
3. 'Operator': objects take in take in a 2D meshgrid (x, y) , source-detector distance d , as well as an input f , and return the operation $\text{PSF}(d) [f'(x, y, d)]$

Kernel1D objects can be constructed using a variety of functions. For example, the `__init__` method of `FunctionKernel1D` requires a 1D function definition $k(x)$, an amplitude function $A(d, b_A)$ and its hyperparameters b_A , and a scaling function $\sigma(d, b_\sigma)$ and its hyperparameters b_σ . The `__call__` method returns $A(d, b_A)k(x/\sigma(d, b_\sigma))\Delta x$ where Δx is the spacing of the kernel. Kernel1D objects require a `normalization_constant(x, d)` method to be implemented that returns sum of the kernel from $x = -\infty$ to $x = \infty$ at each detector distance d given x input with constant spacing Δx . This is not as simple as summing over the kernel output since the range of x provided might be less than the size of the kernel. Kernel2D objects are analogous to Kernel1D objects, except they take in a 2D input (x, y) and return a corresponding 2D kernel at each detector distance d .

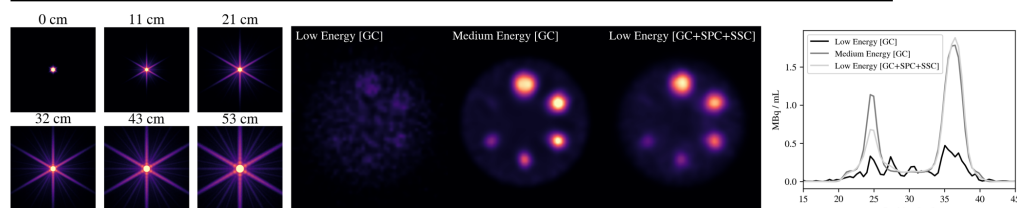
Operator objects are the main component of the library; specific subclasses of operators can be built using Kernel1D and Kernel2D objects. Currently, the library has support for linear shift invariant (LSI) operators, since these are nearly always used for SPECT PSF modeling. LSI operators can always be implemented via convolution with a 2D kernel, but often this is computationally expensive. In tutorial 5, the form of the SPECT PSF is exploited and a 2D LSI operator is built using 1D convolutions and rotations. In tutorial 7, this is shown to lead to faster reconstruction than application of a 2D convolution but with nearly the same results. Operators must also implement a `normalization_constant(xv, yv, d)` method. The `__add__` and `__mult__` methods of operators have been implemented so that multiple PSF operators can be chained together; adding operators together yields an operator that returns the sum of the two PSFs applied to the input data, while multiplying operators yields an operator that returns successive operation of the PSFs applied to the input data. Propagation of normalization is implemented to ensure the normalization of the chained operator is properly implemented. In a gamma camera, for example, there are two components of the PSF: (i) blurring induced from the collimator and (ii) blurring induced from the intrinsic resolution of the scintillator crystals. Provided each operator is instantiated as `psf_coll` and `psf_scint` respectively, the chained PSF operator is `psf_tot=psf_scint*psf_coll`; the `__call__` method of this operator implements

$$\text{PSF}_{\text{total}} [f] = \text{PSF}_{\text{scint}} [\text{PSF}_{\text{coll}} [f]] \quad (2)$$

84 The library is demonstrated using two use cases via reconstruction with the ordered subset
 85 expectation maximum (OSEM) algorithm (Hudson & Larkin, 1994). The first use case considers
 86 reconstruction of MC ^{177}Lu data. ^{177}Lu is typically acquired using a medium energy collimator
 87 and the PSF is dominated by the GC. When acquired using a low energy collimator, there is
 88 significant SPC and SSC, and a more sophisticated PSF model is required during reconstruction.
 89 This use case considers a cylindrical phantom with standard NEMA sphere sizes filled at a 10:1
 90 source to background concentration with a total activity of 1000 MBq. SPECT acquisition
 91 was simulated in SIMIND (Ljungberg & Strand, 1989) using (i) low energy collimators and (ii)
 92 medium energy collimators with 96 projection angles at $0.48\text{ cm} \times 0.48\text{ cm}$ resolution and a
 93 128×128 matrix size. Firstly, each case was reconstructed with GC PSF modeling (Gaussian
 94 PSF) with OSEM(4it,8ss) (medium energy) and OSEM(40it8ss) (low energy). A MC based
 95 PSF model that encompasses GC, SPC, and SSC was then obtained by (i) simulating a point
 96 source at 1100 distances between 0 cm and 55cm, and normalizing the kernel data and (ii)
 97 using a NearestKernelOperator which convolves the PSF kernel closest to the source-detector
 98 distance of each plane. The low energy collimator data was then reconstructed using the MC
 99 PSF model using OSEM (40it8ss). Figure 1 shows the sample PSF at six sample distances
 100 (left), the reconstructed images (center) and sample 1D profiles of the reconstructed images
 101 (right). When the MC PSF kernel that includes GC+SSC+SPC is used, the activity in the
 102 spheres is significantly higher than when the GC only (Gaussian) kernel is used.

103 The second use case considers reconstruction of MC ^{225}Ac data. ^{225}Ac emits 440keV photons
 104 that have significant SPC and SSC even when a high energy collimator is used. This use
 105 case considers a cylindrical phantom with 3 spheres of diameters 60mm, 37mm, and 28mm
 106 filled at a 6.4:1 source to background ratio with 100MBq of total activity. 440keV point
 107 source data was simulated via SIMIND at 1100 positions between 0cm and 55cm. 12 of these
 108 positions were used for developing and fitting a PSF operator built using the GaussianOperator,
 109 Rotate1DConvOperator, and RotateSeperable2DConvOperator; each of these classes performs
 110 2D shift invariant convolutions using only 1D convolutions and rotations (1D-R). More details
 111 on this model and how it is fit are shown in tutorial 5 on the GitHub page. The developed
 112 model is compared to a MC based model (2D) that uses the NearestKernelOperator with the
 113 1100 acquired PSFs acquired from SIMIND. Use of the 1D-R model in image reconstruction
 114 reduces the required computation time by a factor of 2.5, since rotations and 1D convolutions
 115 are significantly faster than direct 2D convolution, even when fast fourier transform techniques
 116 are used.

Lu177 Reconstruction: Low vs. Medium Energy Collimators



Ac225 Reconstruction: High Energy Collimator PSF Modeling

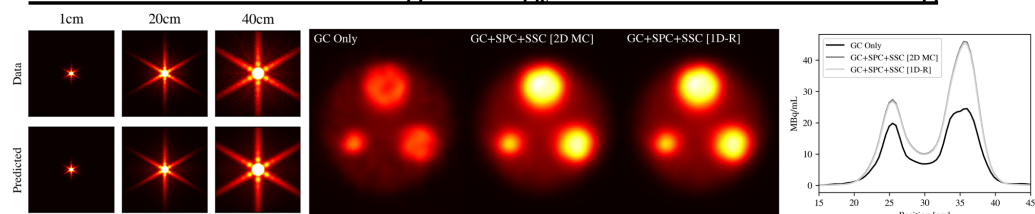


Figure 1: Upper: ^{177}Lu reconstruction example. From left to right: MC PSF data at various source detector distances, axial slices from reconstructions, and central vertical 1D profile from shown axial slices. Lower: ^{225}Ac reconstruction example. From left to right: MC PSF data and predicted 1D-R fit, axial slices from reconstructions, and central vertical 1D profile from shown axial slices.

References

- Barrett, H. H., Myers, K. J., & Dhurjaty, S. (2003). Foundations of image science. *J. Electronic Imaging*, 14, 029901. <https://api.semanticscholar.org/CorpusID:206393854>
- Delker, A., Schleske, M., Liubchenko, G., & others. (2023). Biodistribution and dosimetry for combined $[^{177}\text{Lu}]\text{u-PSMA-i\&t}/[^{225}\text{Ac}]\text{ac-PSMA-i\&t}$ therapy using multi-isotope quantitative SPECT imaging. *European Journal of Nuclear Medicine and Molecular Imaging*, 50, 1280–1290. <https://doi.org/10.1007/s00259-022-06092-1>
- Hudson, H. M., & Larkin, R. S. (1994). Accelerated image reconstruction using ordered subsets of projection data. *IEEE Transactions on Medical Imaging*, 13(4), 601–609. <https://doi.org/10.1109/42.363108>
- Kratochwil, C., & others. (2018). Targeted α -therapy of metastatic castration-resistant prostate cancer with $^{225}\text{Ac-PSMA-617}$: Swimmer-plot analysis suggests efficacy regarding duration of tumor control. *Journal of Nuclear Medicine*, 59(5), 795–802.
- Liubchenko, G., & others. (2024). Image-based dosimetry for $[^{225}\text{Ac}]\text{ac-PSMA-i\&t}$ therapy and the effect of daughter-specific pharmacokinetics. *European Journal of Nuclear Medicine and Molecular Imaging*, 51(8), 2504–2514. <https://doi.org/10.1007/s00259-024-06681-2>
- Ljungberg, M., & Strand, S.-E. (1989). A monte carlo program for the simulation of scintillation camera characteristics. *Computer Methods and Programs in Biomedicine*, 29(4), 257–272. [https://doi.org/https://doi.org/10.1016/0169-2607\(89\)90111-9](https://doi.org/https://doi.org/10.1016/0169-2607(89)90111-9)
- Polson, L., Fedrigo, R., Li, C., Sabouri, M., Dzikunu, O., Ahamed, S., Karakatsanis, N., Rahmim, A., & Uribe, C. (2024). *PyTomography: A python library for quantitative medical image reconstruction*. <https://arxiv.org/abs/2309.01977>
- Rosar, F., & others. (2021). Molecular imaging and biochemical response assessment after a single cycle of $[^{225}\text{Ac}]\text{ac-PSMA-617}/[^{177}\text{Lu}]\text{u-PSMA-617}$ tandem therapy in mCRPC patients who have progressed on $[^{177}\text{Lu}]\text{u-PSMA-617}$ monotherapy. *Theranostics*, 11(9), 4050.

- 143 Sathekge, M., & others. (2020). Predictors of overall and disease-free survival in metastatic
144 castration-resistant prostate cancer patients receiving 225Ac-PSMA-617 radioligand therapy.
145 *Journal of Nuclear Medicine*, 61(1), 62–69.
- 146 Zacherl, M. J., & others. (2021). First clinical results for PSMA-targeted α -therapy using
147 225Ac-PSMA-i&t in advanced-mCRPC patients. *Journal of Nuclear Medicine*, 62(5),
148 669–674.

DRAFT