

Nuts & Bolts of Advanced Imaging

The Image Reconstruction Pipeline

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23rd Annual Meeting

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SMRT 24th Annual Meeting • 30–31 May

Toronto, Ontario, Canada

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Declaration of Financial Interests or Relationships

Speaker Name: Michael S. Hansen

I have the following financial interest or relationship to disclose with regard to the subject matter of this presentation:

Company Name: Siemens Medical Solutions

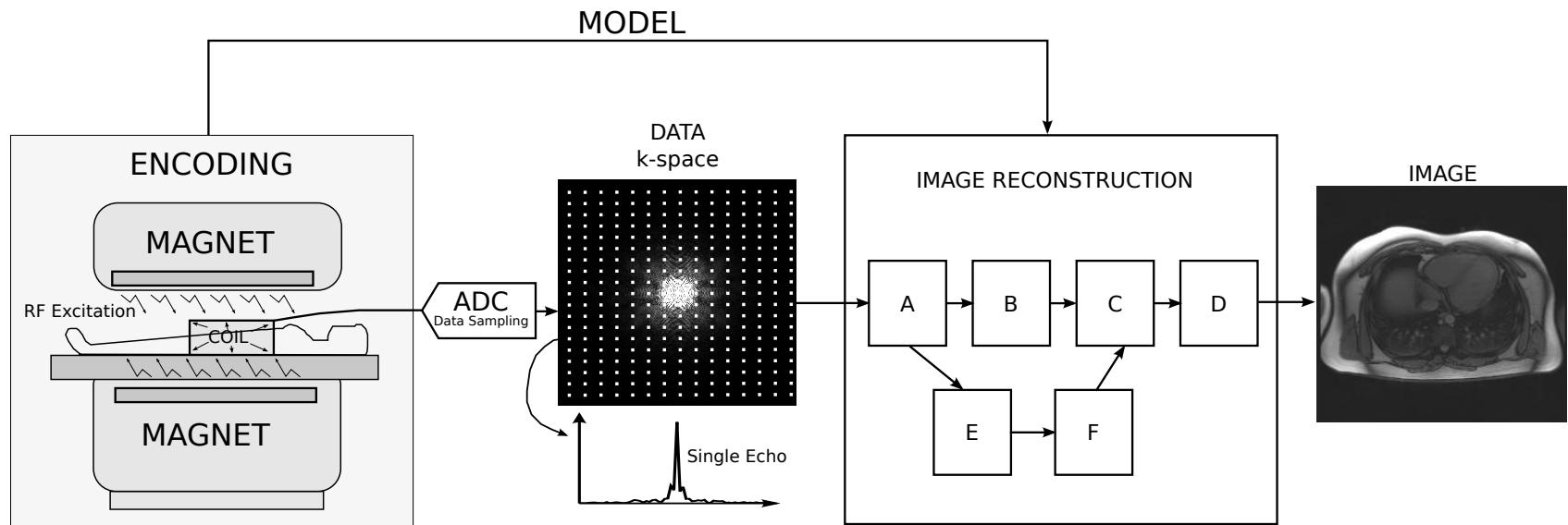
Type of Relationship: Research Agreement

Outline

- What is a reconstruction pipeline
- Common pipeline elements:
 - Noise adjust, filtering, accumulation, FFT
- A Simple Reconstruction Pipeline Example
 - Cartesian Parallel Imaging
- Examples of pipeline architectures
 - Open Source
 - Vendors

PART 1

The role of the image reconstruction process



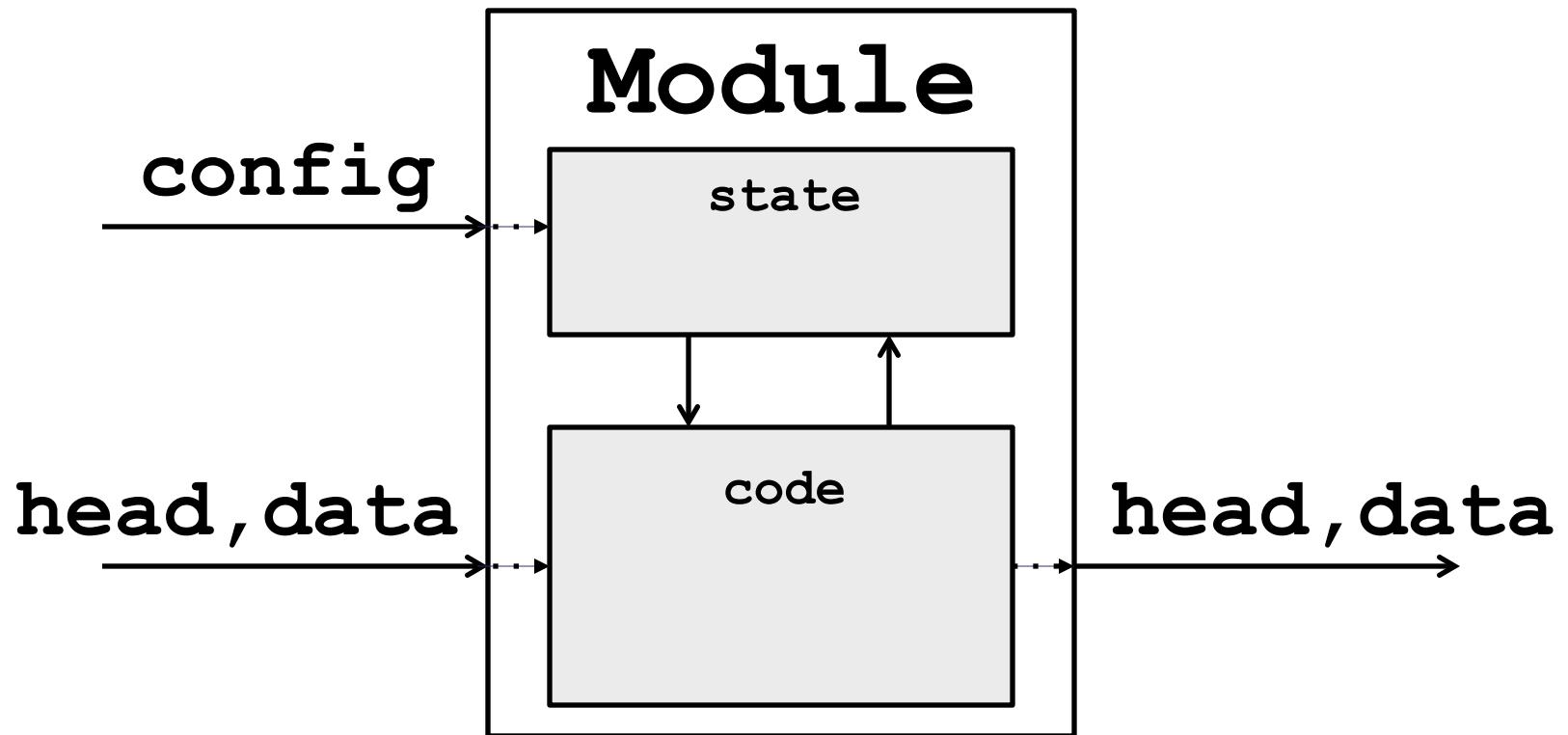
Reconstruction Pseudo Code

```
function reconstruct(datafile) :
```

Problems with the `reconstruct` function

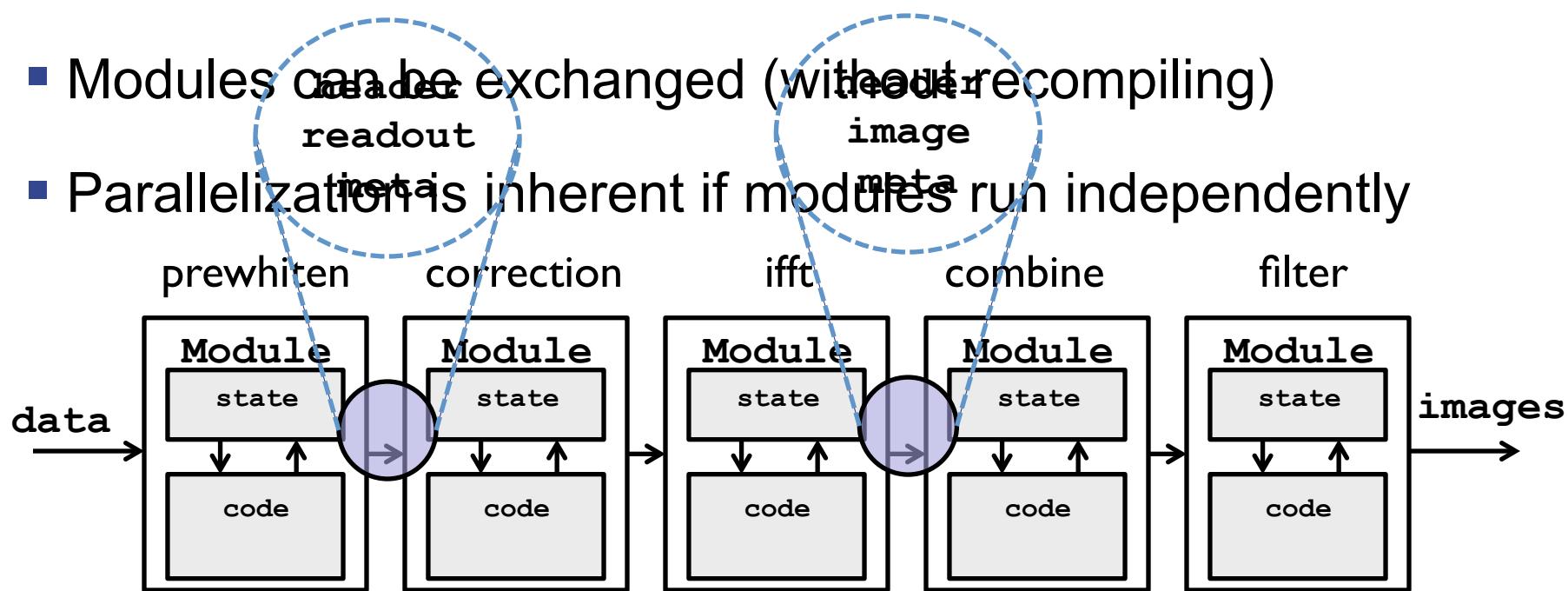
- Reconstruction does not start until all data is stored
- Parallelization requires low level management
- Changes to reconstruction software requires editing of source code function (and recompilation of code)
- Encourages bad programming practices:
 - Poorly defined data structures (interfaces)
 - Duplication of code

A modular pipeline

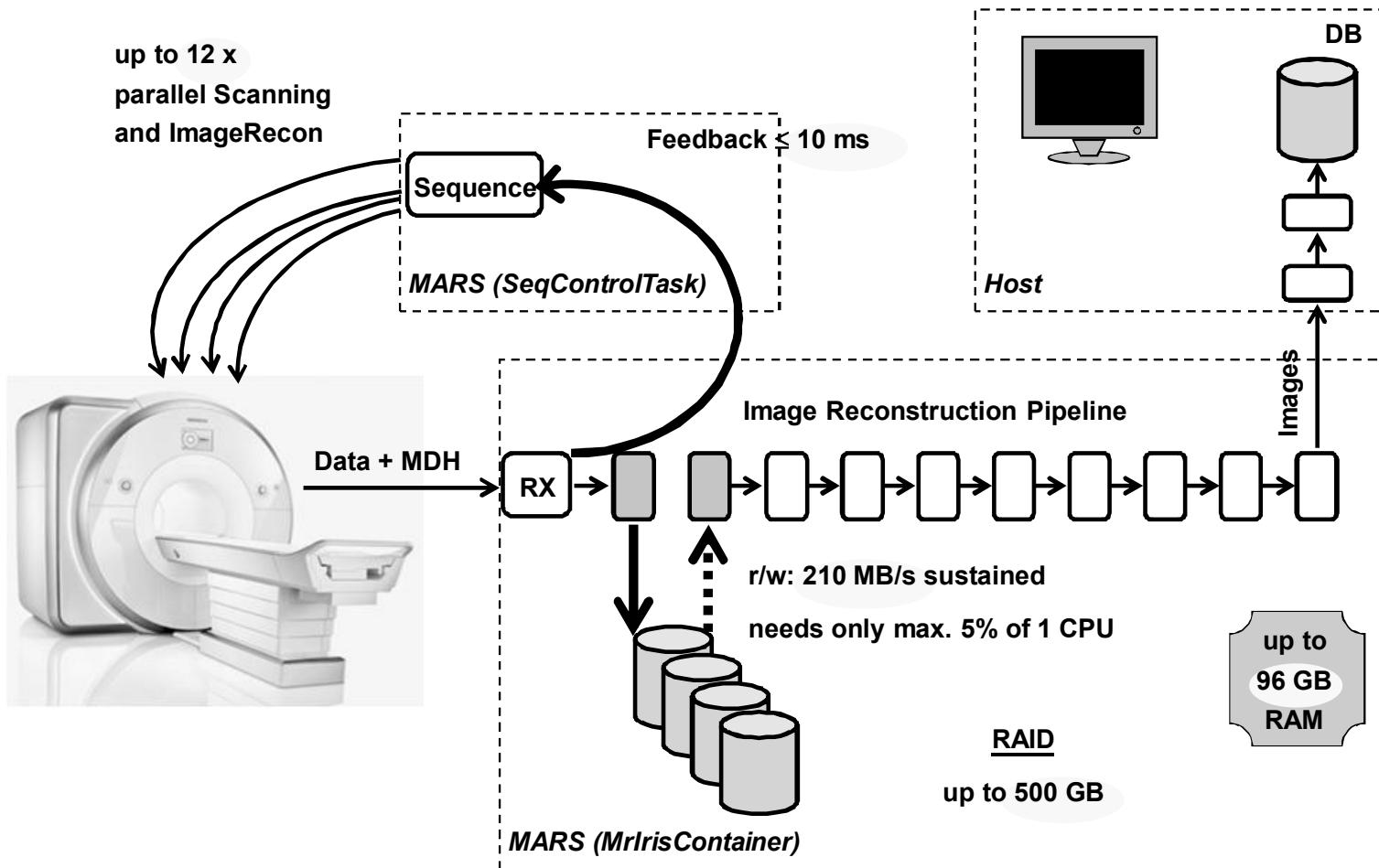


A modular pipeline

- Modular reconstruction design
- Well defined interfaces and data structures
- Processing can start when first readout is acquired
- Modules can be exchanged (without recompiling)
- Parallelization is inherent if modules run independently

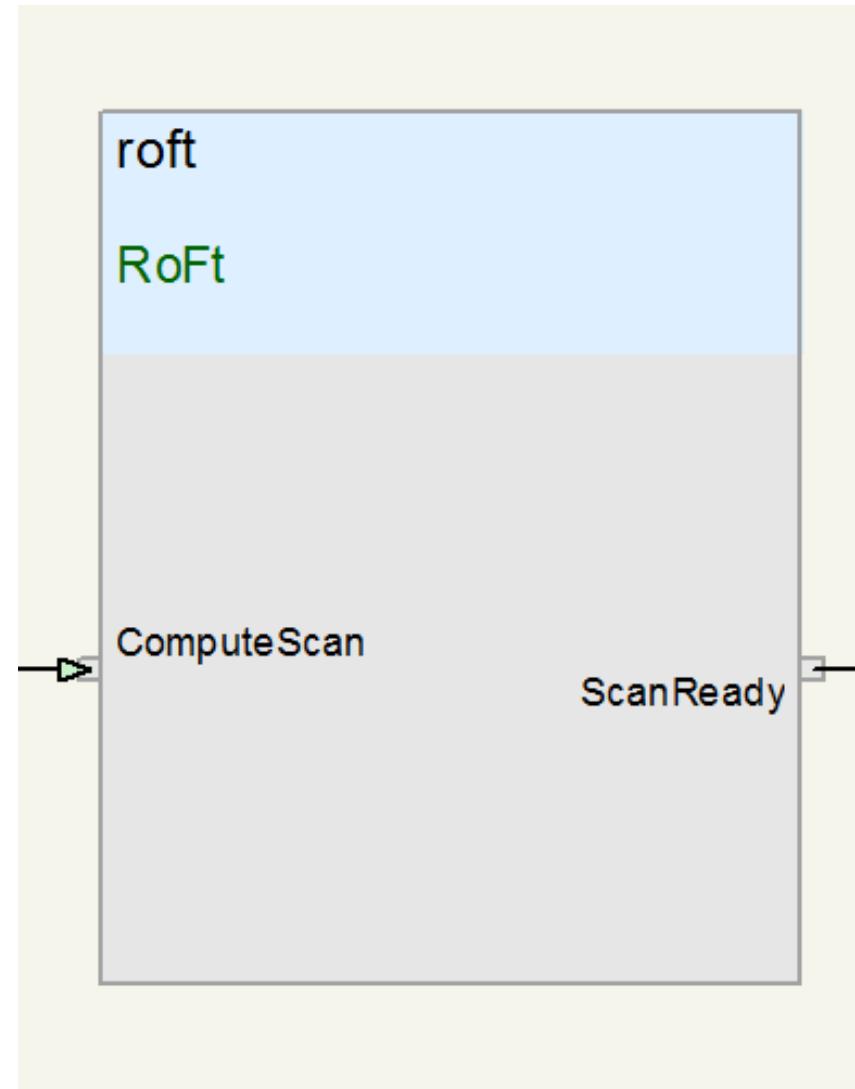


Siemens Reconstruction Pipeline



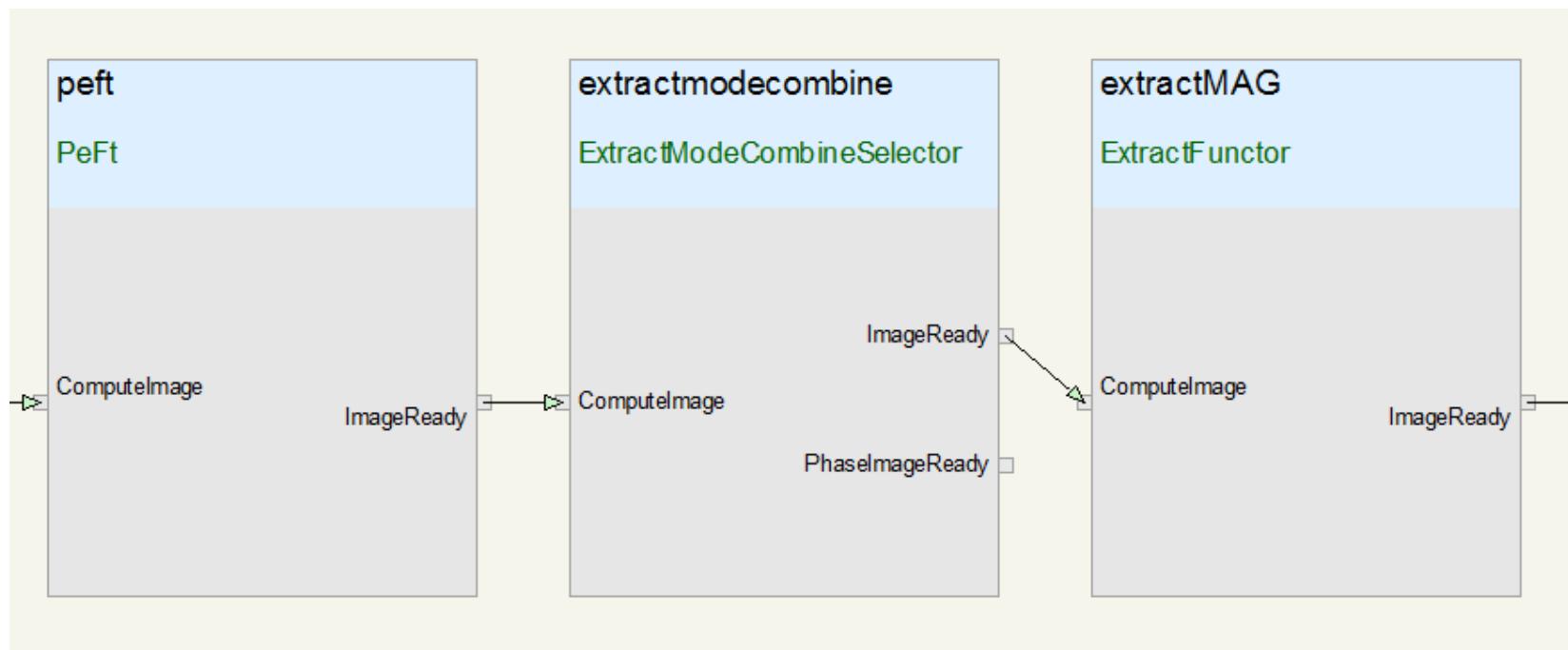
Functor

- Modules are called functors.
- Data structures are well defined on interfaces.
- Modules are interchangeable.
- Configured at run time.



Functor Chain

The user interfaces with the underlying framework through specification of a file known as the Ice program. This program specifies the functor chain of operations and configuration parameters, based upon the type of pulse sequence and the desired data output (integer images, complex raw data).



The Basics of a Reconstruction Application

Data Sorting and Organization

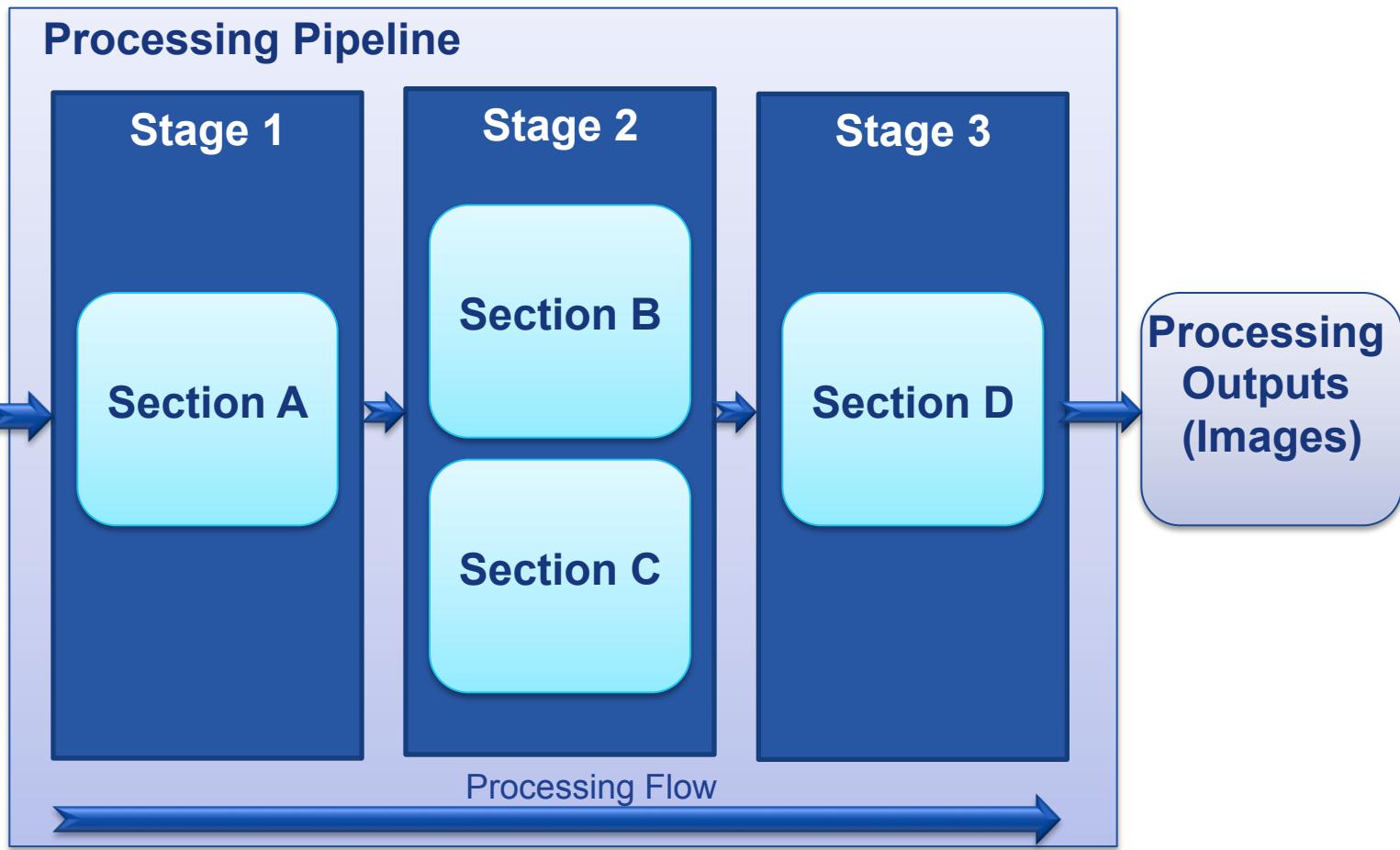
- Meaningful data structure based on application or desired processing
- Raw acquisition data can be: scanner, raw files, data streams

Processing Pipeline

- Group of **Processing Sections**: Modules that typically “do math” and have custom inputs/output
- The pipeline builds and wires the **Sections** in **stages** that define the processing **flow**
- Pipeline building defines:
 - Processing order
 - Section dependencies
 - Distribution of processing



Example



Programming Window: The Orchestra SDK

Collection of modular and reusable **product** recon algorithms

- MATLAB functions
- C++ classes and functions

DICOM Toolbox

- Create, read, and write compliant files
- Store/stream images to networked peers

Multi-Platform

- Linux, Mac, Windows

Raw file readers

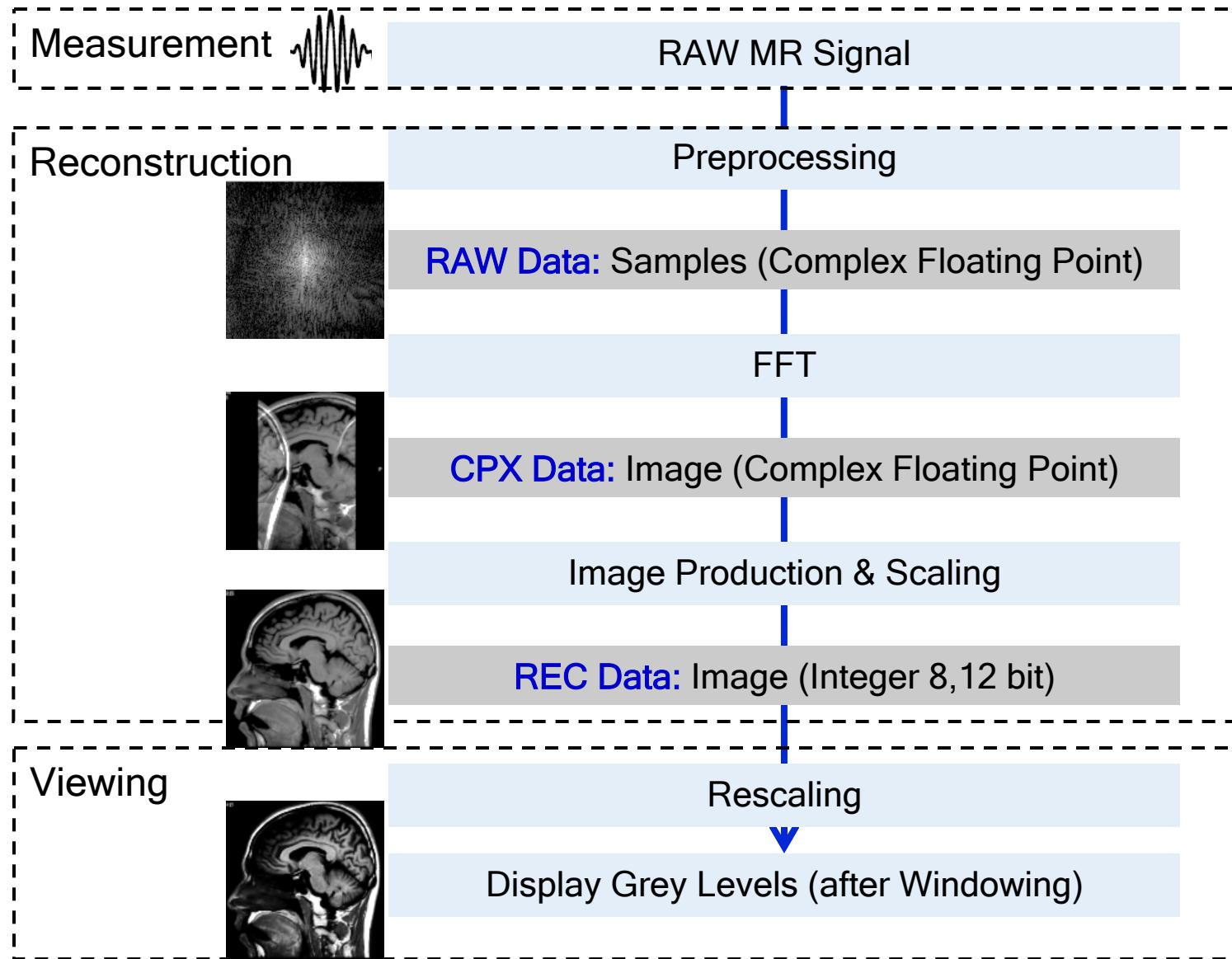
- APIs for accessing data and parameters

GE example pipelines

- Cartesian, EPI, Spectroscopy



Data Stream



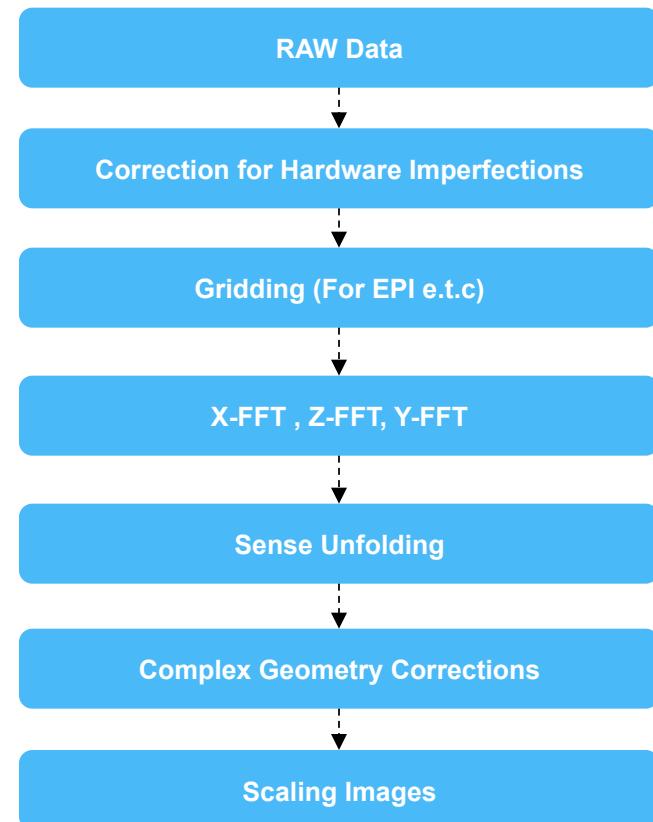
Introduction to Recon 2.0

Nodes, Reconstruction Graph

Reconstruction is a sequence of steps for transforming data received from the previous step and passing it onto the next step.

Nodes The individual steps performed in the reconstruction pipeline are referred to as Nodes.

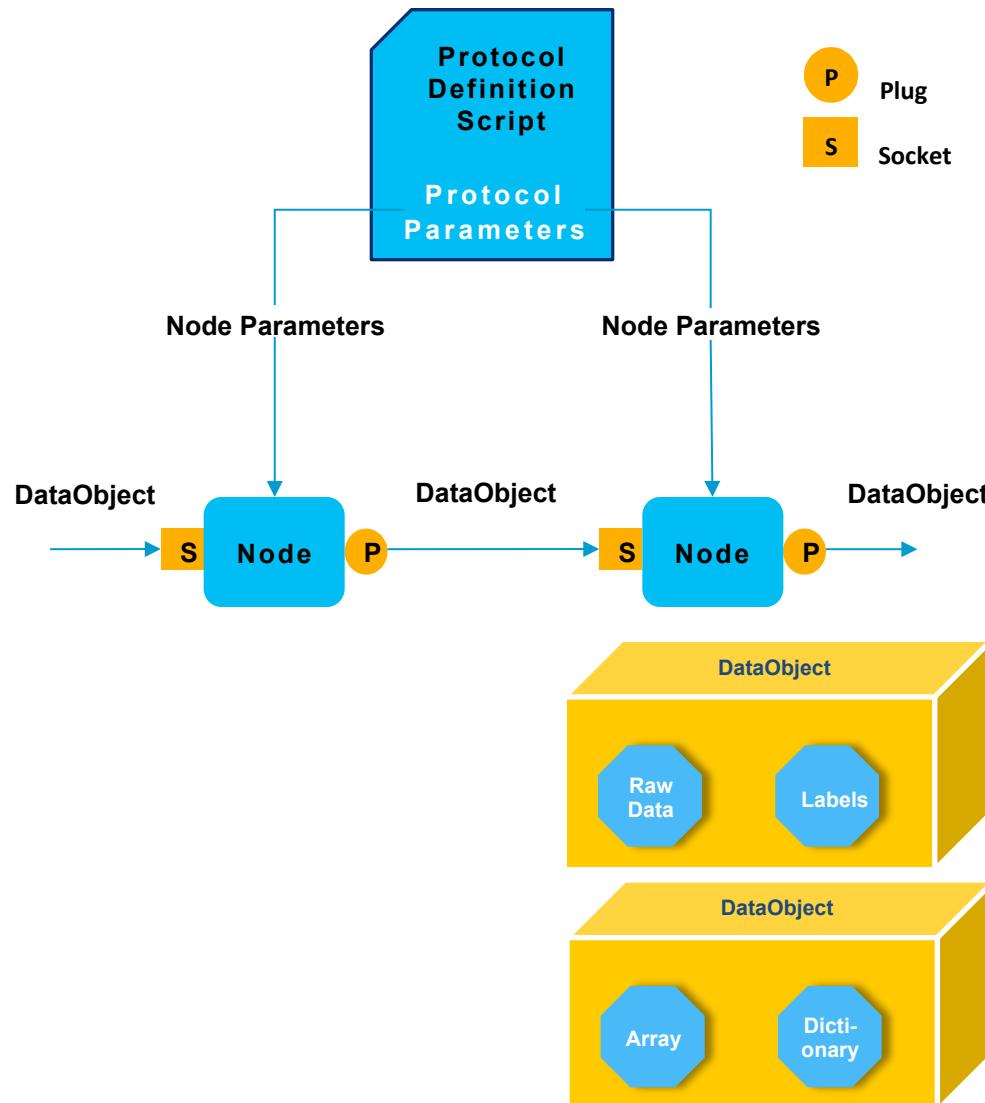
Reconstruction Graph The pipeline connecting the nodes to each other is called as the reconstruction graph.



- ready-to-use platform for complete MR image reconstruction
- raw data processed via independent, easy to adapt processing modules called “nodes”

Introduction to Recon 2.0

Framework Architecture



Summary

- Modern reconstruction software is often implemented as streaming pipeline architectures
 - Modularity
 - Performance
- Modules have well defined data interfaces and are interchangeable to some extend
- Modules can often be assembled at run-time to form different recon programs (without recompilation)

What to expect in Part 2

- We will play with a simple recon pipeline:
 - Built in Python
 - Basic Parallel Imaging reconstruction
- Open Raw Data Standard
 - ISMRMRD
- Open Source Pipeline Environments
 - Gadgetron
 - GPI
 - Codeare

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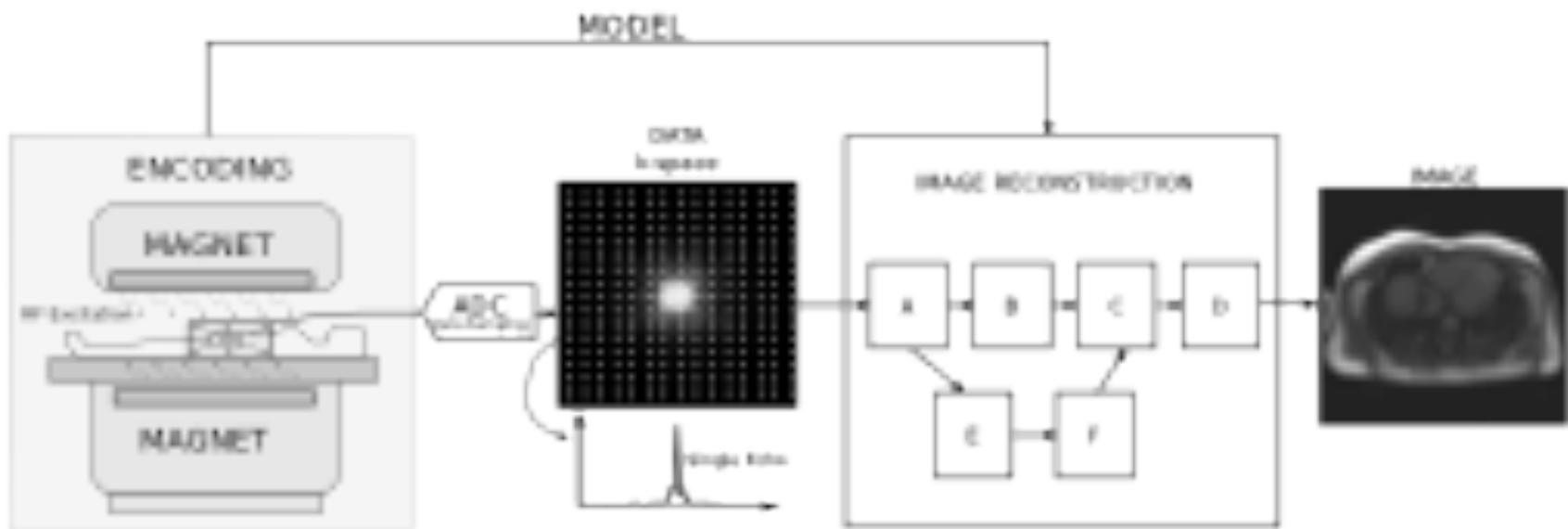
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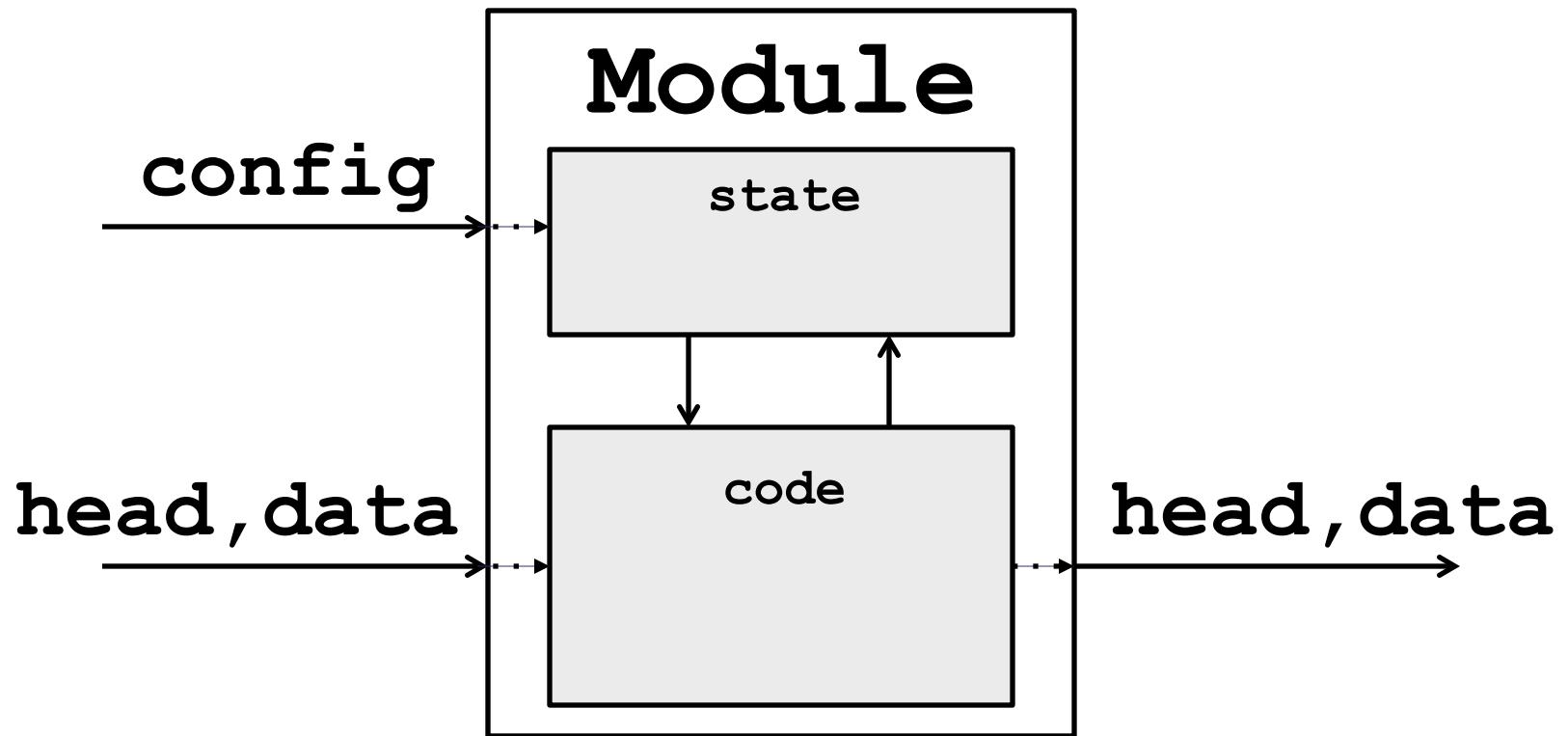
Type of Relationship: Research Agreement

PART 2

The role of the image reconstruction process

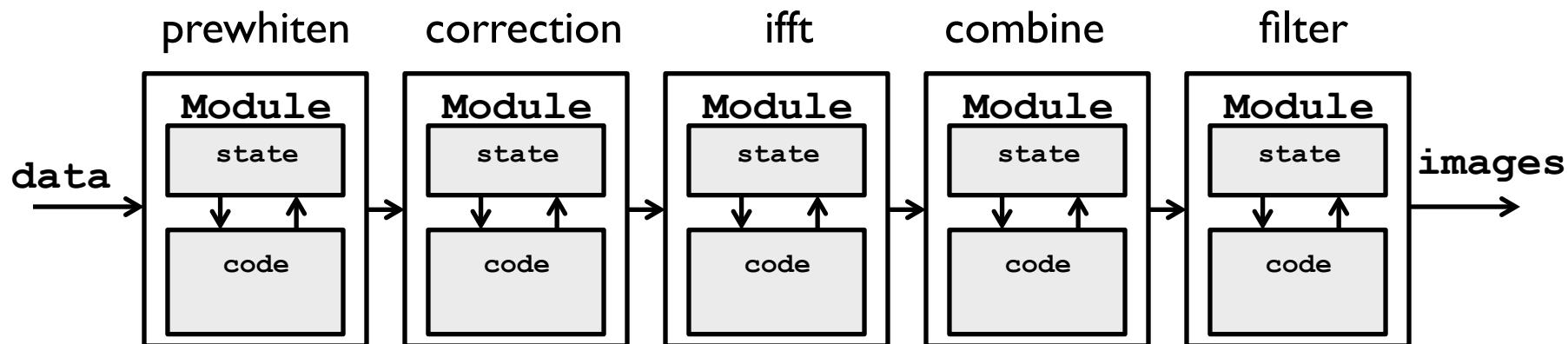


A modular pipeline



A modular pipeline

- Modular reconstruction design
- Well defined interfaces and data structures
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Implement 2D Cartesian Parallel Imaging

Magnetic Resonance in Medicine 42:952–962 (1999)

SENSE: Sensitivity Encoding for Fast MRI

Klaas P. Pruessmann, Markus Weiger, Markus B. Scheidegger, and Peter Boesiger*

New theoretical and practical concepts are presented for considerably enhancing the performance of magnetic resonance imaging (MRI) by means of arrays of multiple receiver coils. Sensitivity encoding (SENSE) is based on the fact that the signal generally has an encoding effect during preparation by linear field gradients. By using receiver coils in parallel scan considerably reduced. The problem of how to reconstruct from sensitivity encoded data is solved and solved for arbitrary coil coupling patterns. Special attention is given to a practical case, namely, sampling at a reduced density. For this case methods was verified both in vivo and in phantom experiments.

Therefore, samples of distinct information content can be obtained at one time by using distinct receivers in parallel (2), implying the possibility of reducing scan time in

Magnetic Resonance in Medicine 47:1202–1210 (2002)

Generalized Autocalibrating Partially Parallel Acquisitions (GRAPPA)

Mark A. Griswold,^{1*} Peter M. Jakob,¹ Robin M. Heidemann,¹ Mathias Nittka,² Vladimir Jellus,² Jianmin Wang,² Berthold Kiefer,² and Axel Haase¹

In this study, a novel partially parallel acquisition (PPA) method is presented which can be used to accelerate image acquisition using an RF coil array for spatial encoding. This technique, Generalized Autocalibrating Partially Parallel Acquisitions (GRAPPA) is an extension of both the PILS and VD-AUTO-SMASH reconstruction techniques. As in those previous methods, a detailed, highly accurate RF field map is not needed prior to reconstruction in GRAPPA. This information is obtained from several k -space lines which are acquired in addition to the normal image acquisition. As in PILS, the GRAPPA reconstruction algorithm provides unaliased images from each component coil prior to image combination. This results in even higher SNR and better image quality since the steps of image recon-

actual coil sensitivity information is difficult to determine experimentally due to contamination by, for example, noise. Additionally, subject or coil motion between the time of coil calibration and image acquisition can be problematic if this information is not taken into account during the reconstruction.

Last year, we presented the parallel imaging with localized sensitivities (PILS) technique (14) and demonstrated several advantages. In PILS it is assumed that each component coil has a localized sensitivity profile. Whenever this is true, uncombined coil images can be formed for each component coil using only knowledge of the position

Cartesian Parallel Imaging - Ingredients

1. Data
2. Software

Details and code: <http://hansenms.github.io/sunrise>

ISMRM Raw Data Format

HDF5 File Container

XML Header

```
<?xml version="1.0" encoding="UTF-8" standalone="no" ?>
<ismrmdHeader xmlns="http://www.ismrm.org/ISMRRMD"
  xmlns:xsi="http://www.w3.org/2001/XMLSchema-instance"
  xsi:schemaLocation="http://www.ismrm.org/ISMRRMD ismrmd.xsd">

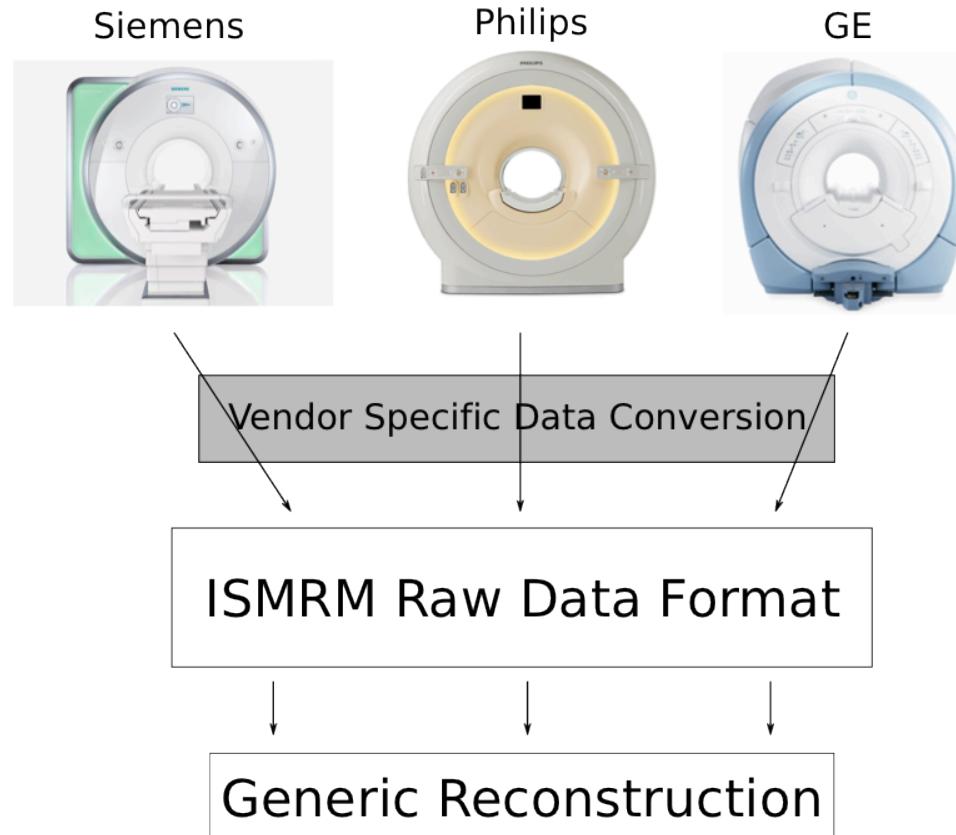
<encoding>
  <encodedSpace>
    <matrixSize>
      <x>512</x><y>256</y><z>1</z>
    </matrixSize>
    <fieldOfView_mm>
      <x>600</x><y>300</y><z>6</z>
    </fieldOfView_mm>
  </encodedSpace>
  <reconSpace>
    <matrixSize>
      <x>256</x><y>256</y><z>1</z>
    </matrixSize>
    <fieldOfView_mm>
      <x>300</x><y>300</y><z>6</z>
    </fieldOfView_mm>
  </reconSpace>
  <encodingLimits>
    <kspace_encoding_step_1>
      <minimum>0</minimum>
      <maximum>255</maximum>
      <center>128</center>
    </kspace_encoding_step_1>
    <repetition>
      <minimum>0</minimum>
      <maximum>1</maximum>
      <center>0</center>
    </repetition>
  </encodingLimits>
  <trajectory>cartesian</trajectory>
</encoding>

</ismrmdHeader>
```

Raw Data

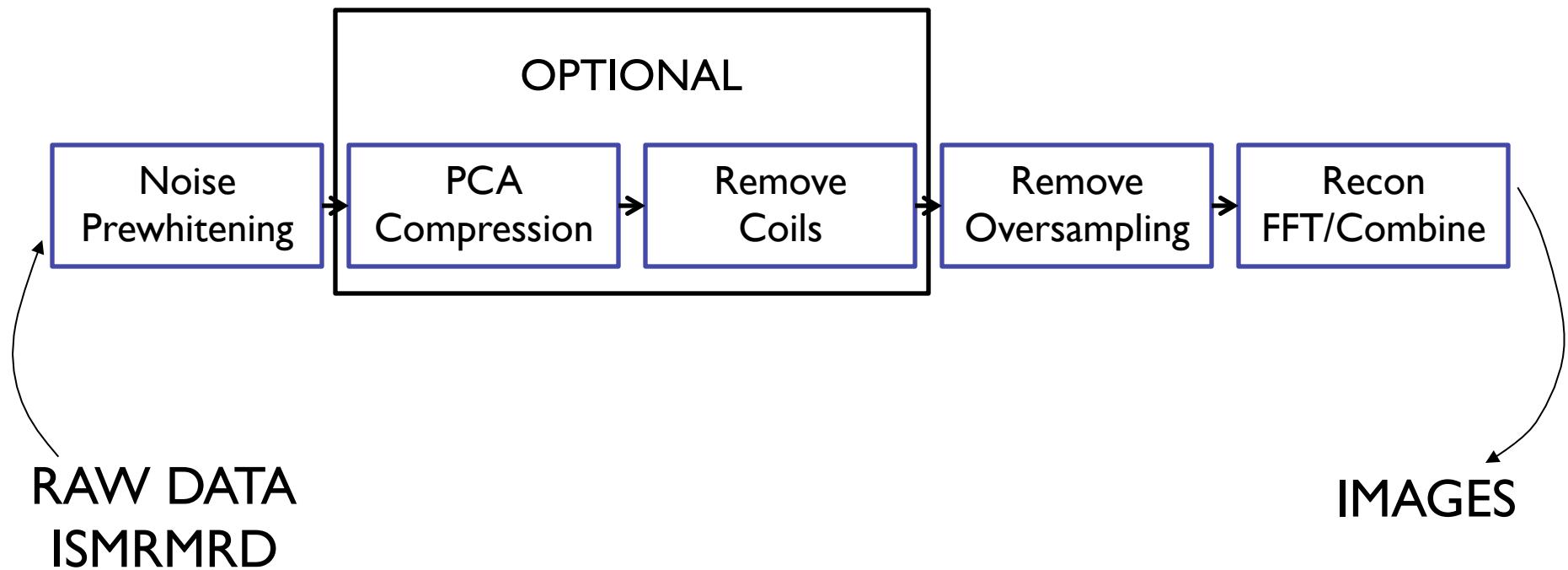
http://ismrmrd.github.io

ISMRM Raw Data Format



Info on converters: michael.hansen@nih.gov

Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA



Pipeline Module (aka Gadget, Node, Functor, etc.)

class Module/Gadget/Functor:

- state (member variables, buffers, etc.)
- next module
- `process_config(conf)`
 - sets up the module
 - uses general header information
- `process(head, data, meta)`
 - processes actual data
 - operates on one data element at a time

Loop counter information
Timing information

Sampled data
Image data

OPTIONAL
Data labels
Image labels
Calculated timing
Scaling information
Etc.

Some example Python code

```
import ismrmrd
import ismrmrd.xsd
from gadgetron import gadget_chain_wait
from gadgetron import gadget_chain_config
from tpat_snr_scale import RemOS, NoiseAdj, PCA, CoilReduce, Recon
```

```
def define_gadget_chain():
    g2 = Recon()
    g1 = RemOS(next_gadget=g2)
    g0 = CoilReduce(next_gadget=g1)
    gb = PCA(next_gadget=g0)
    ga = NoiseAdj(next_gadget=gb)
    return ga

g_python = define_gadget_chain()
```

SET UP MODULES

```
dset = ismrmrd.Dataset(filename, 'dataset', create_if_needed=False)
```

OPEN DATASET

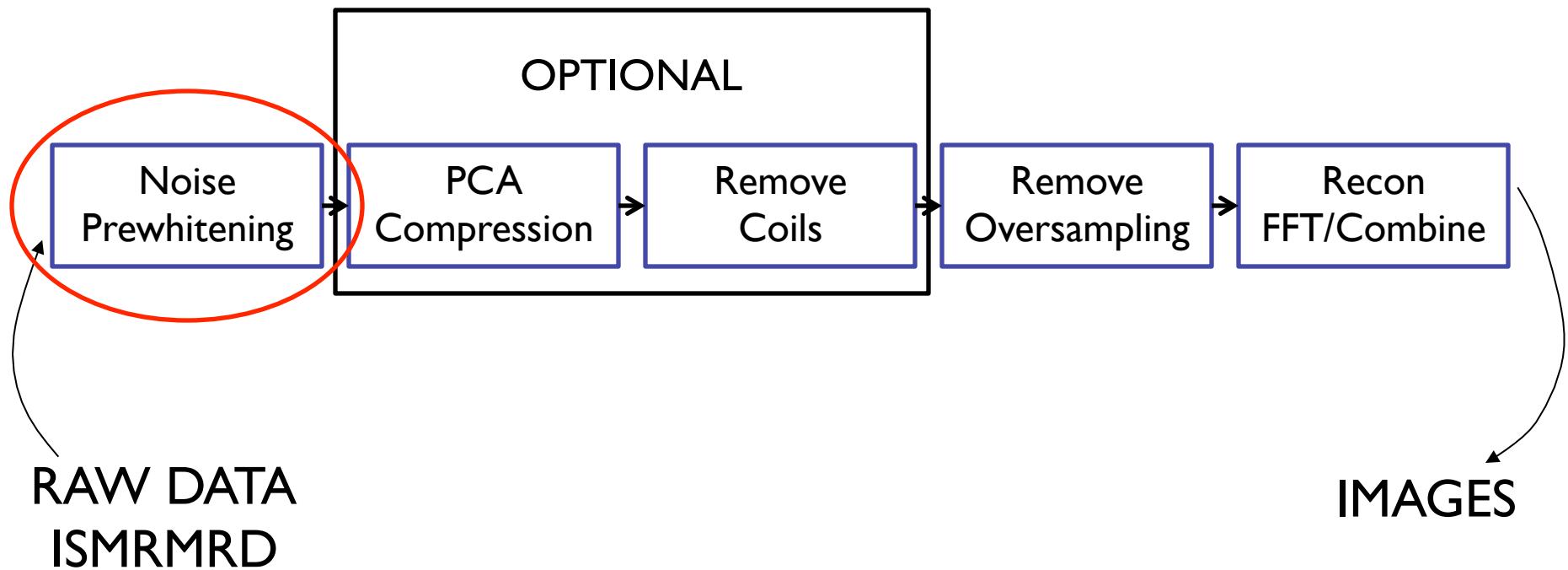
```
# Send in data
#First ISMRMRD XML header
gadget_chain_config(g_python,dset.read_xml_header())

# Loop through the rest of the acquisitions and stuff
for acqnum in range(0,dset.number_of_acquisitions()):
    acq = dset.read_acquisition(acqnum)
    g_python.process(acq.getHead(),acq.data.astype('complex64'))

# Wait for recon to finish
gadget_chain_wait(g_python)
```

RECONSTRUCT

Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA



Noise in Parallel Imaging

Idealized Experiment:

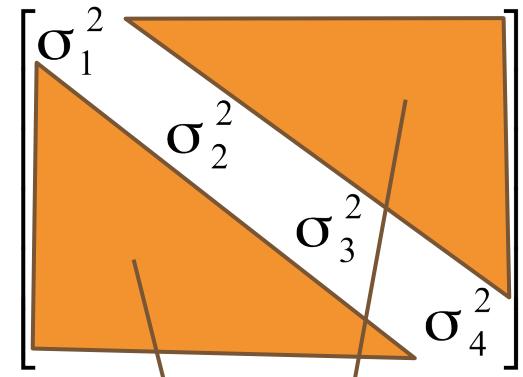
$$\mathbf{s} = \mathbf{E}\rho$$

In practice, we are affected by noise

$$\mathbf{s} = \mathbf{E}\rho + \boldsymbol{\eta}$$

Noise covariance matrix

$$\Psi_{Y,Y'} = \langle \boldsymbol{\eta}_Y, \boldsymbol{\eta}_{Y'} \rangle$$



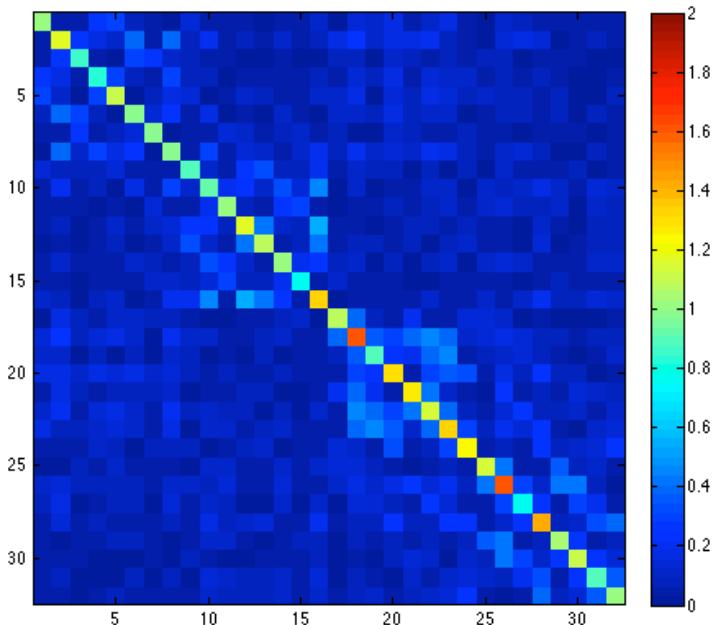
We can measure this noise covariance:

```
# Python
% eta: [Ncoils, Nsamples]
Psi = (1/(M-1))*np.asmatrix(eta)*np.asmatrix(eta).H
```

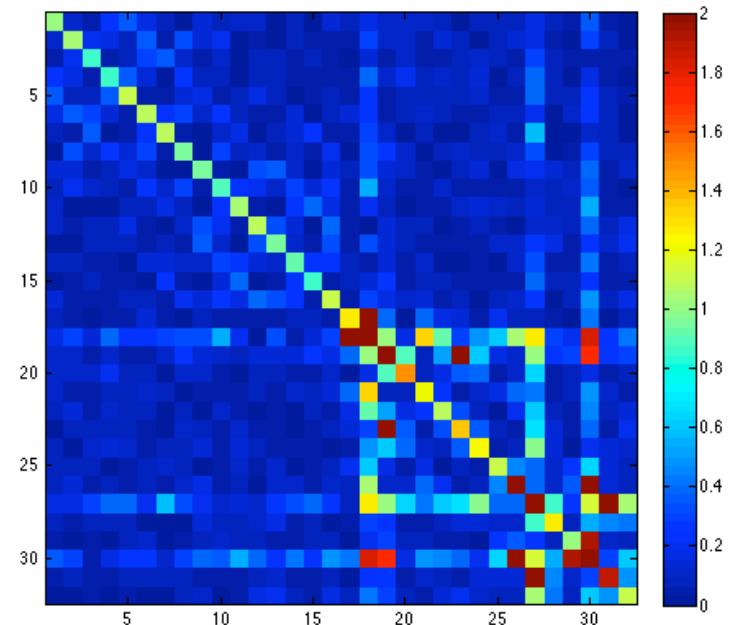
Noise correlation

Psi Examples – 32 Channel Coil

“Normal Coil”



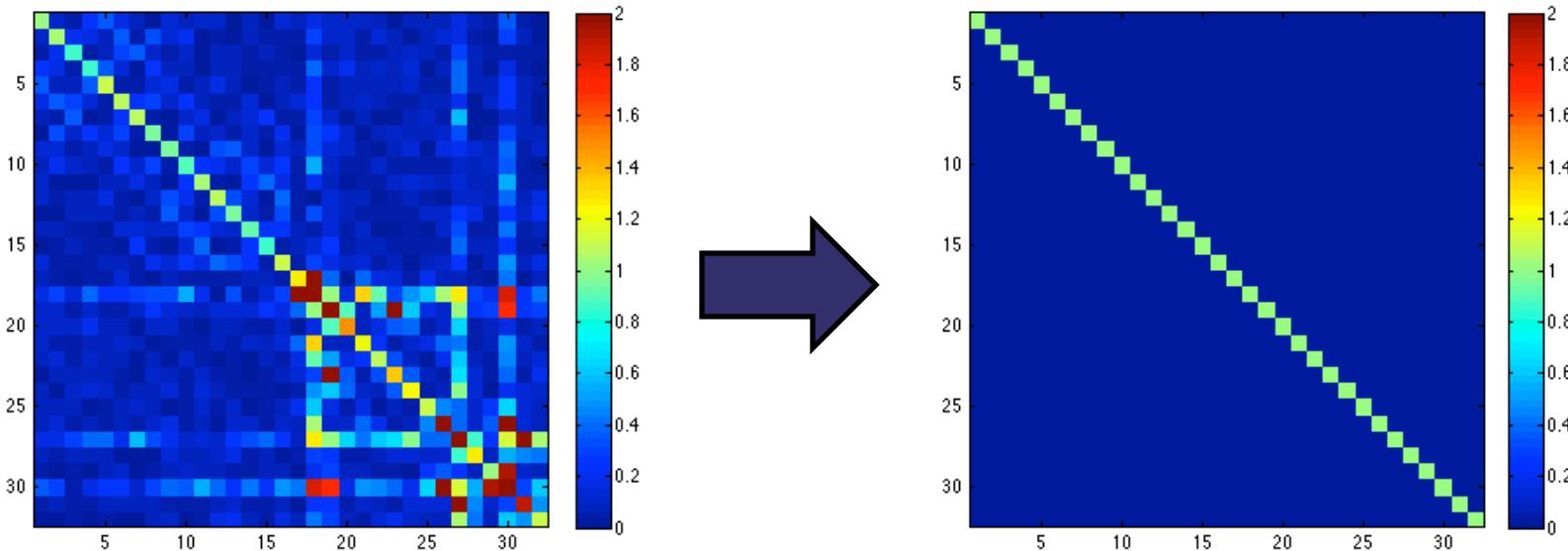
“Broken Coil”



Examination of the noise covariance matrix is an important QA tool. Reveals broken elements, faulty pre-amps, etc.

Noise Pre-Whitening

We would like to apply an operation such that we have unit variance in all channels:



Noise Pre-Whitening

More generally, we want to weight the equations with the “inverse square root” of the noise covariance, if

$$\Psi = \mathbf{L}\mathbf{L}^H$$

We will solve:

$$\mathbf{L}^{-1}\mathbf{A}\mathbf{x} = \mathbf{L}^{-1}\mathbf{b}$$

Or:

$$\mathbf{x} = (\mathbf{A}^H \Psi^{-1} \mathbf{A})^{-1} \mathbf{A}^H \Psi^{-1} \mathbf{b}$$

In practice, we simply generate “pre-whitened” input data before recon

Noise Prewhitening - Python Code

```
import numpy as np

def calculate_prewhitenning(noise, scale_factor=1.0):
    '''Calculates the noise prewhitening matrix

    :param noise: Input noise data (array or matrix), ``[coil, nsamples]``
    :param scale_factor: Applied on the noise covariance matrix. Used to
        adjust for effective noise bandwidth and difference in
        sampling rate between noise calibration and actual measurement:
        scale_factor = (T_acq_dwell/T_noise_dwell)*NoiseReceiverBandwidthRatio

    :returns w: Prewhitenning matrix, ``[coil, coil]``, w*data is prewhitened
    '''

    noise_int = noise.reshape((noise.shape[0],noise.size/noise.shape[0]))
    M = float(noise_int.shape[1])
    dmtx = (1/(M-1))*np.asmatrix(noise_int)*np.asmatrix(noise_int).H
    dmtx = np.linalg.inv(np.linalg.cholesky(dmtx));
    dmtx = dmtx*np.sqrt(2)*np.sqrt(scale_factor);
    return dmtx

def apply_prewhitenning(data,dmtx):
    '''Apply the noise prewhitening matrix

    :param noise: Input noise data (array or matrix), ``[coil, ...]``
    :param dmtx: Input noise prewhitening matrix

    :returns w_data: Prewhitenned data, ``[coil, ...]``,
    '''

    s = data.shape
    return np.asarray(np.asmatrix(dmtx)*np.asmatrix(data.reshape(data.shape[0],data.size/data.shape[0]))).reshape(s)
```

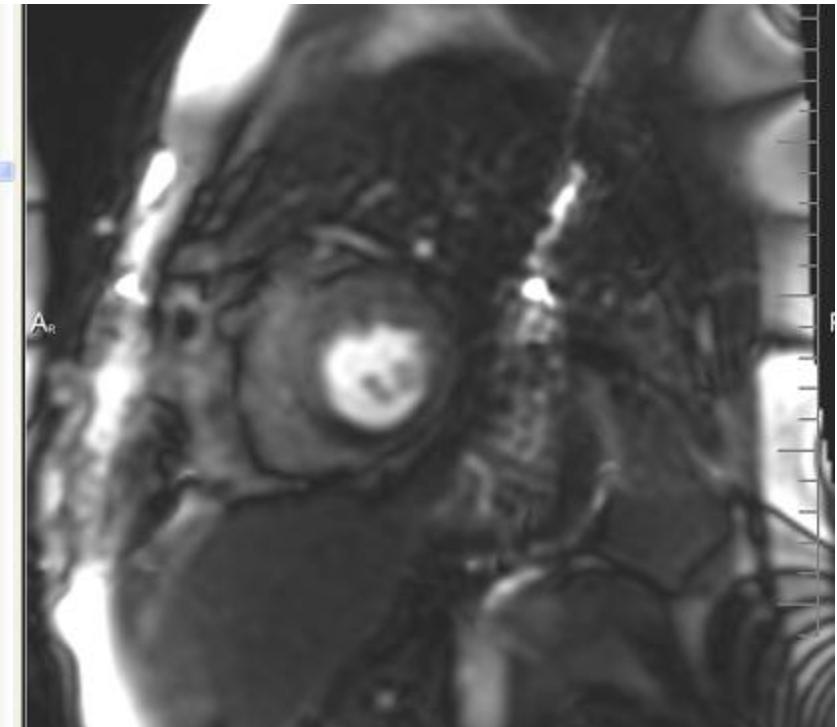
Noise Pre-Whitening – In vivo example

In vivo stress perfusion case where broken coil element resulted in non-diagnostic images.

Without pre-whitening



With pre-whitening



Example provided by Peter Kellman, NIH

Noise Adjust Module

```
class NoiseAdj(Gadget):
    def __init__(self, next_gadget = None):
        Gadget.__init__(self, next_gadget)
        self.noise_data = list()
        self.noise_dmtx = None
    def process(self,acq,data,*args):
        if acq.isFlagSet(ismrmmrd.ACQ_IS_NOISE_MEASUREMENT):
            self.noise_data.append((acq,data))
        else:
            if len(self.noise_data):
                profiles = len(self.noise_data)
                channels = self.noise_data[0][1].shape[0]
                samples_per_profile = self.noise_data[0][1].shape[1]
                noise = np.zeros((channels,profiles*samples_per_profile),dtype=np.complex64)
                counter = 0
                for p in self.noise_data:
                    noise[:,counter*samples_per_profile:(counter*samples_per_profile+samples_per_profile)] = p[1]
                    counter = counter + 1

                scale = (acq.sample_time_us/self.noise_data[0][0].sample_time_us)*0.79
                self.noise_dmtx = coils.calculate_prewhitenning(noise,scale_factor=scale)

                #Test the noise adjust
                d = self.noise_data[0][1]
                d2 = coils.apply_prewhitenning(d, self.noise_dmtx)
                self.noise_data = list()

            if self.noise_dmtx is not None:
                data2 = coils.apply_prewhitenning(data, self.noise_dmtx)
            else:
                data2 = data

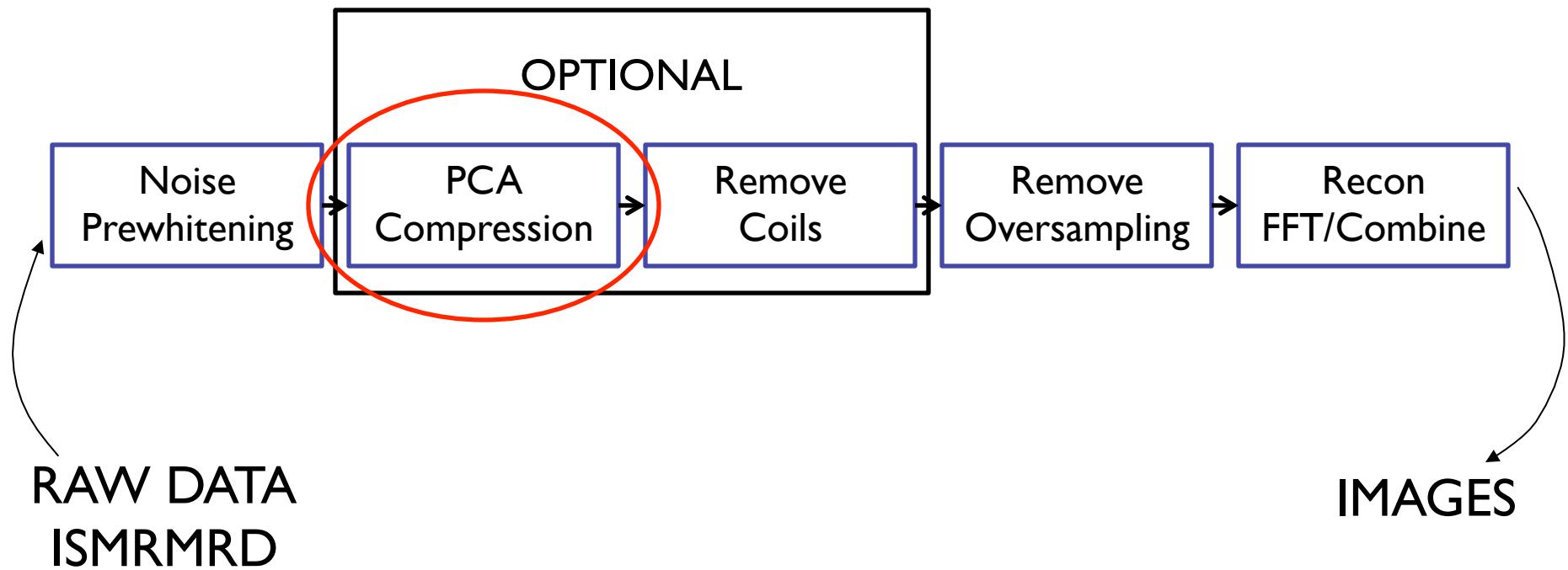
            self.put_next(acq,data2)
    return 0
```

BUFFERING

CALCULATE PREWHITENER

APPLY

Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA



PCA Module

```
class PCA(Gadget):
    def __init__(self, next_gadget=None):
        Gadget.__init__(self, next_gadget)
        self.calib_data = list()
        self.pca_mtx = None
        self.max_calib_profiles = 100
        self.samples_to_use = 16
        self.buffering = True

    def process(self, acq, data, *args):
        if self.buffering:
            self.calib_data.append((acq, data))

        if (len(self.calib_data) >= self.max_calib_profiles or acq.isFlagSet(ismrmrd.ACQ_LAST_IN_SLICE)):
            #We are done buffering calculate pca transformation
            # ...book keeping code (removed to save space, refer to original code)

            A = np.zeros((total_samples, channels), dtype=np.complex64)
            counter = 0
            for p in self.calib_data:
                d = p[1][:, acq.center_sample-(samp_to_use>>1):acq.center_sample+(samp_to_use>>1)]
                A[counter*samp_to_use:counter*samp_to_use+samp_to_use, :] = np.transpose(d)
                counter = counter+1

            m = np.mean(A, 0)
            A_m = A - m.reshape((1, m.shape[0]))
            U, s, V = np.linalg.svd(A_m, full_matrices=False)
            self.pca_mtx = V

            for p in self.calib_data:
                data2 = np.dot(self.pca_mtx, p[1])
                self.put_next(p[0], data2)

            self.buffering = False
            self.calib_data = list()
            return 0
        else:
            if self.pca_mtx is not None:
                data2 = np.dot(self.pca_mtx, data)
                self.put_next(acq, data2, *args)
            else:
                self.put_next(acq, data, *args)

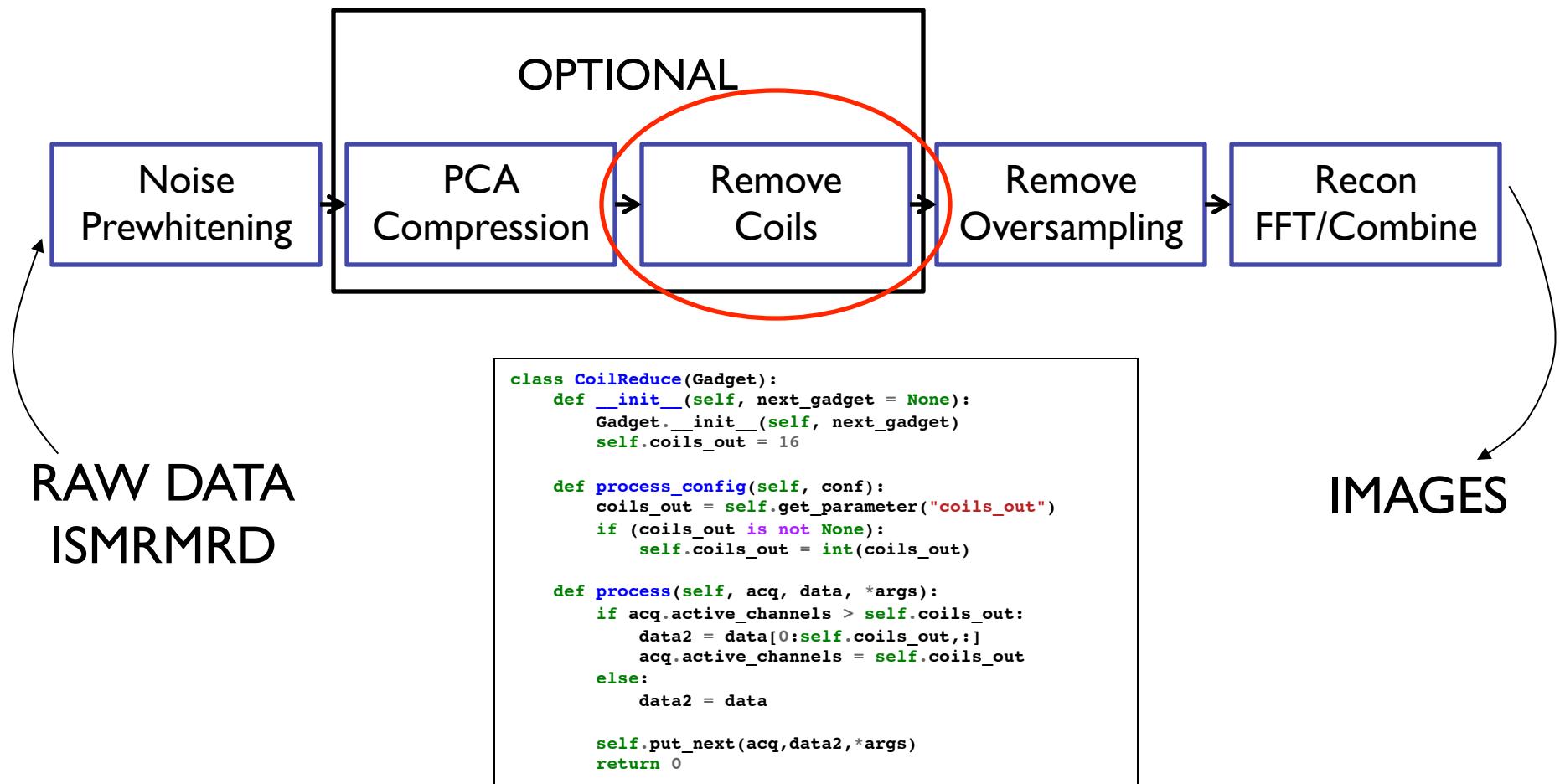
    return 0
```

BUFFERING

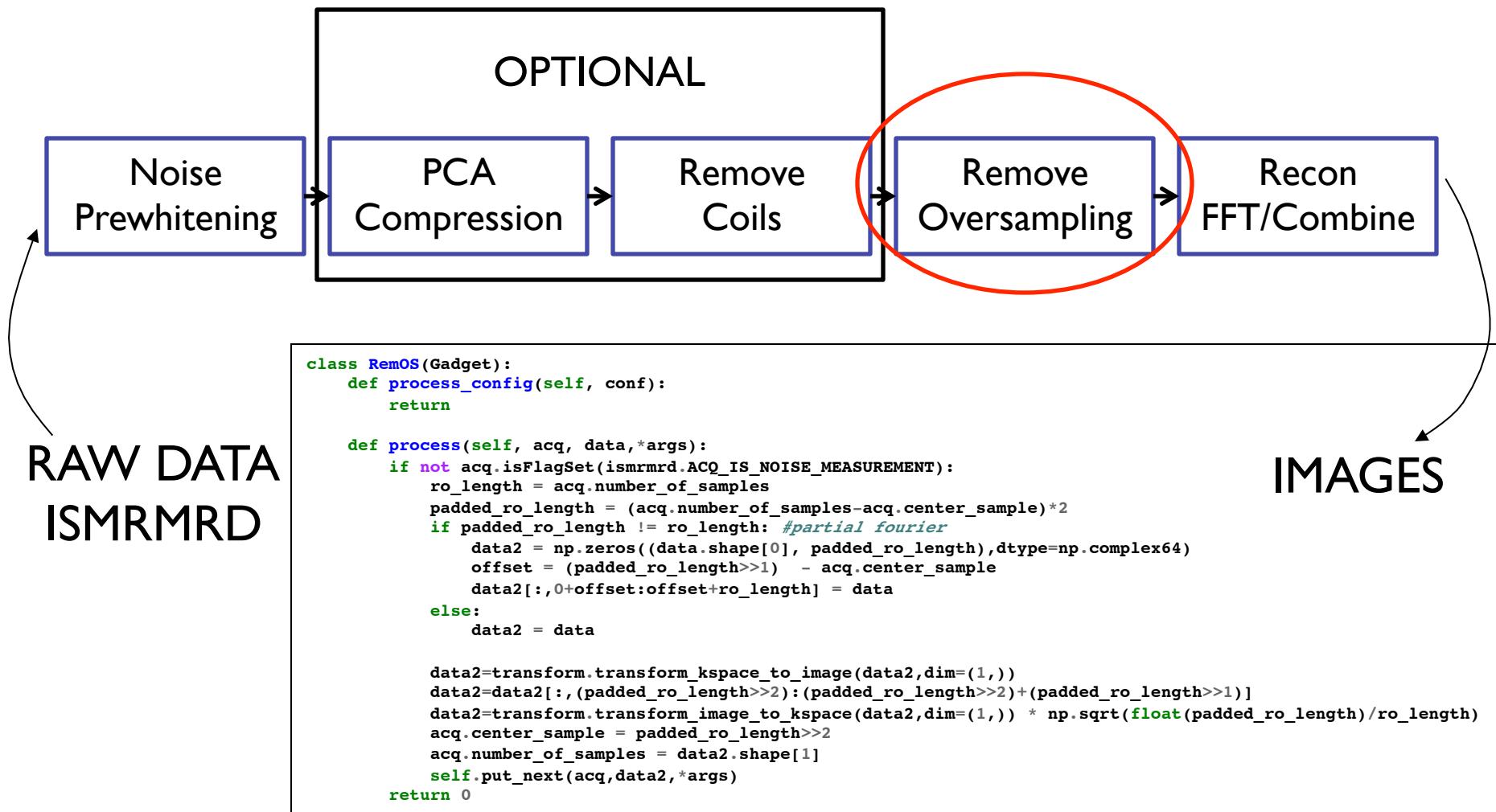
CALCULATE PCA COEFFICIENTS

APPLY

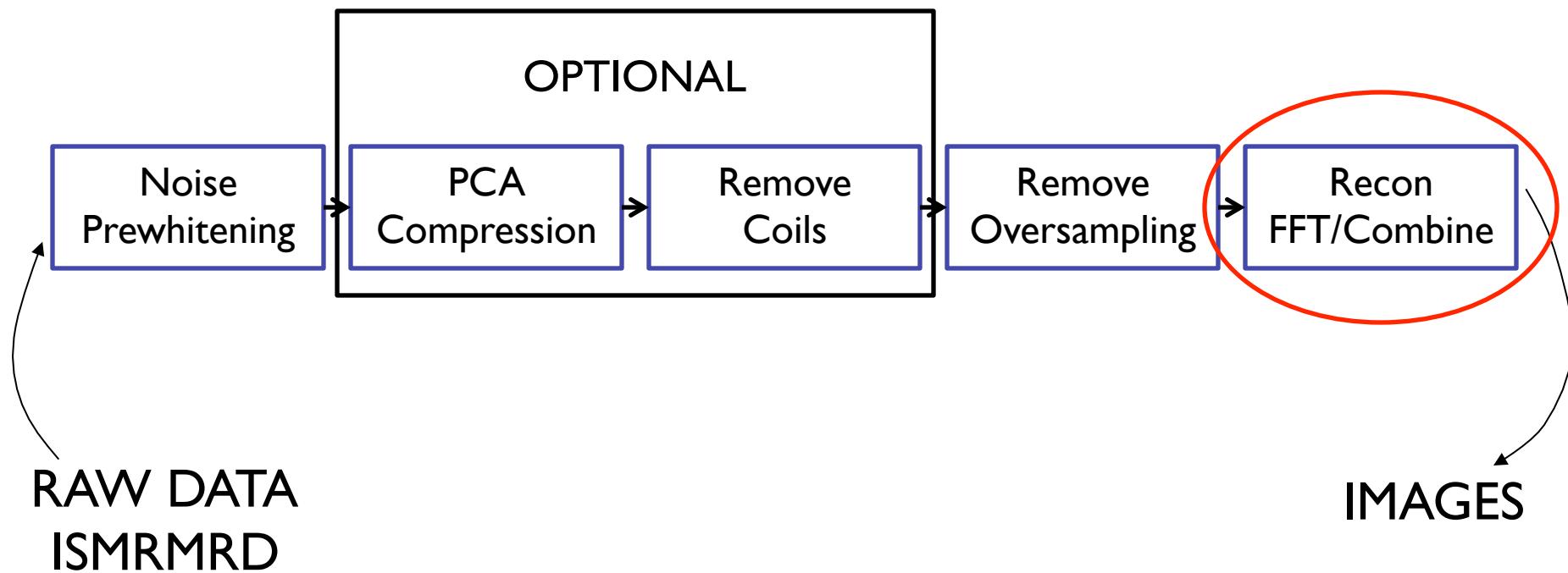
Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA



Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA

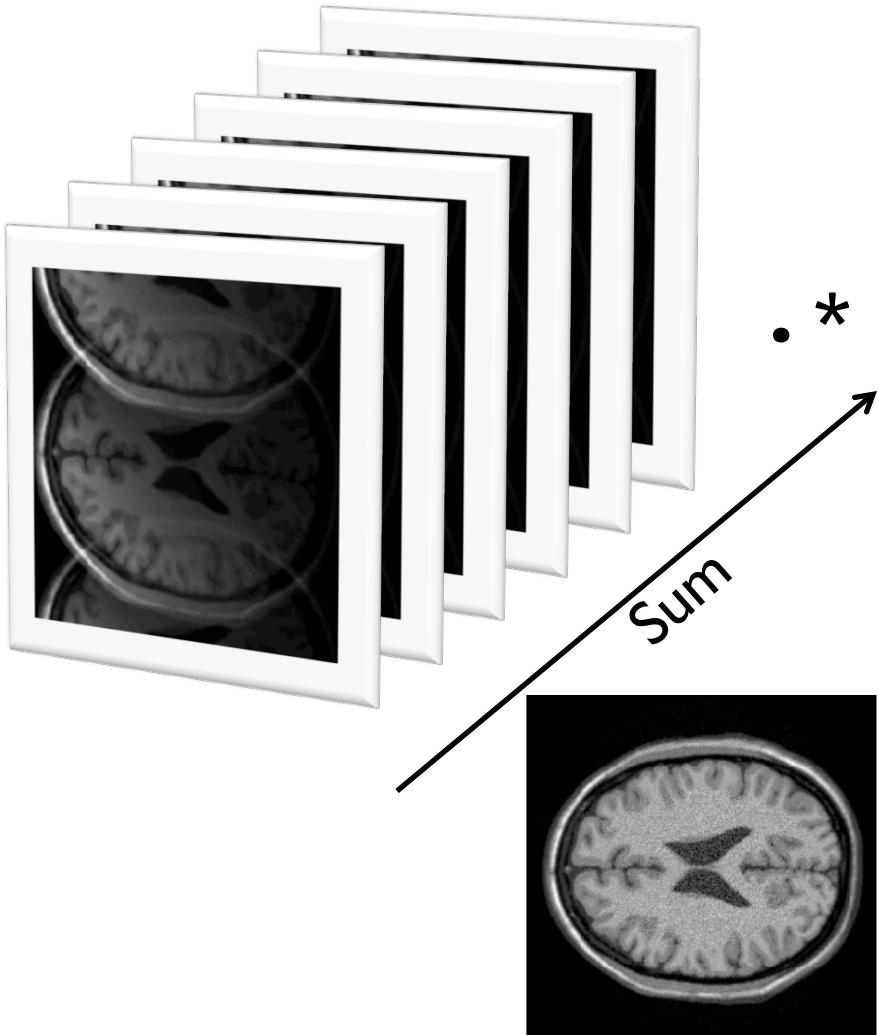


Reconstruction Pipeline – TSENSE, TPAT, TGRAPPA



SENSE – Image Synthesis with Unmixing Coefficients

Aliased coil images

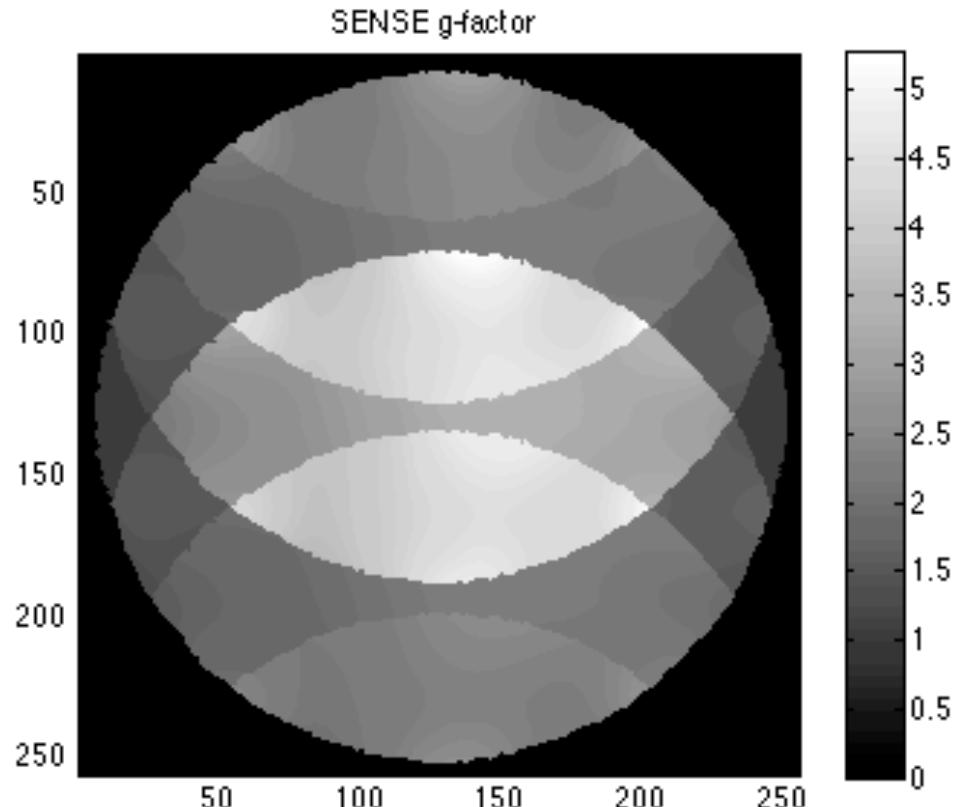
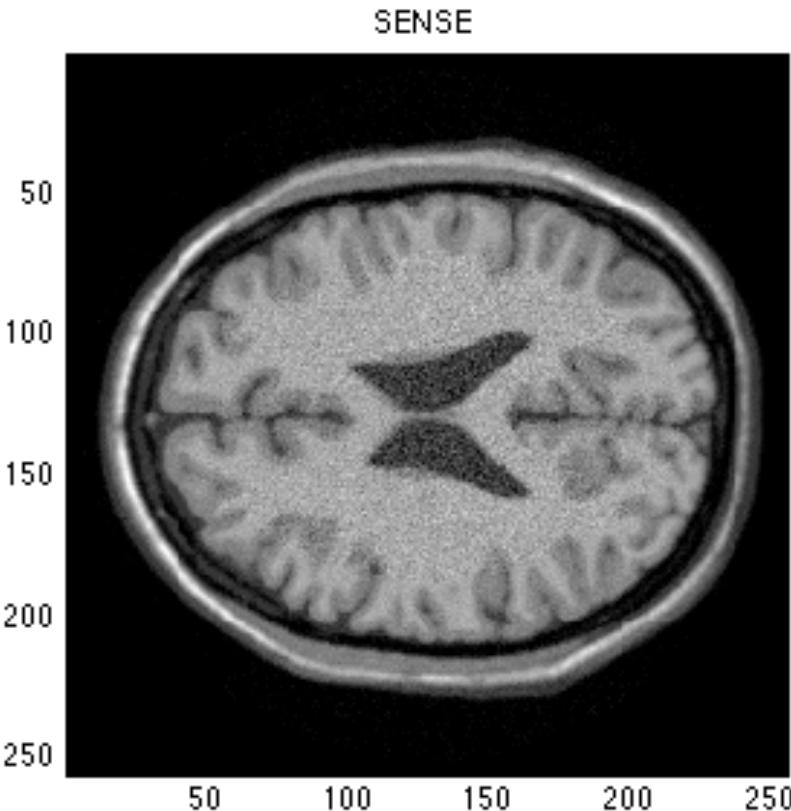


Unmixing Coefficients

SENSE – Simple Rate 4 Example

$$\tilde{\rho}(x_1) = \sum_{i=0}^{N_c} u_i a_i$$

$$g(x_1) = \sqrt{\sum_{i=0}^{N_c} |u_i|^2} \sqrt{\sum_{i=0}^{N_c} |S_i|^2}$$



Recon Module

```
class Recon(Gadget):
    def __init__(self, next_gadget=None):
        Gadget.__init__(self, next_gadget)
        self.header = None
        self.enc = None
        self.acc_factor = None
        self.buffer = None
        self.samp_mask = None
        self.header_proto = None
        self.calib_buffer = list()
        self.unmix = None
        self.gmap = None
        self.calib_frames = 0
        self.method = 'grappa'

    def process_config(self, cfg):
        self.header = ismrrmr.xsd.CreateFromDocument(cfg)
        self.enc = self.header.encoding[0]

        #Parallel imaging factor
        self.acc_factor = self.enc.parallelImaging.accelerationFactor.kspace_encoding_step_1

        reps = self.enc.encodingLimits.repetition.maximum+1
        phs = self.enc.encodingLimits.phase.maximum+1
        if reps > phs:
            self.calib_frames = reps
        else:
            self.calib_frames = phs

        if self.calib_frames < self.acc_factor:
            self.calib_frames = self.acc_factor

        #Frames should be a multiple of the acceleration factor
        self.frames = math.floor(self.calib_frames/self.acc_factor)*self.acc_factor

        pmri_method = self.get_parameter('pmri_method')
        if pmri_method == 'grappa' or pmri_method == 'sense':
            self.method = pmri_method

    def process(self, acq, data,*args):
        ....
```

```

def process_config(self, cfg):
    #...

def process(self, acq, data,*args):

    if self.buffer is None:
        # Matrix size
        # ...initialize buffer (code removed, see original source)

    #Now put data in buffer
    line_offset = self.buffer.shape[1]/2 - self.enc.encodingLimits.kspace_encoding_step_1.
    self.buffer[:,acq.idx.kspace_encode_step_1+line_offset,:] = data
    self.samp_mask[acq.idx.kspace_encode_step_1+line_offset,:] = 1

    #If last scan in buffer, do FFT and fill image header
    if acq.isFlagSet(ismrmrd.ACQ_LAST_IN_ENCODE_STEP1) or acq.isFlagSet(ismrmrd.ACQ_LAST_IN_SLICE):
        #... Set up image header (code removed, see original source)

    #We have not yet calculated unmixing coefficients
    if self.unmix is None:
        self.calib_buffer.append((img_head,self.buffer.copy()))
        self.buffer[:] = 0
        self.samp_mask[:] = 0

        if len(self.calib_buffer) >= self.calib_frames:
            coil_images = transform.transform_kspace_to_image(cal_data,dim=(1,2))
            (csm,rho) = coils.calculate_csm_walsh(coil_images)

            if self.method == 'grappa':
                self.unmix, self.gmap = grappa.calculate_grappa_unmixing(cal_data,
                                                                self.acc_factor,
                                                                kernel_size=(4,5),
                                                                csm=csm)

            elif self.method == 'sense':
                self.unmix, self.gmap = sense.calculate_sense_unmixing(self.acc_factor, csm)
            else:
                raise Exception('Unknown parallel imaging method: ' + str(self.method))

            for c in self.calib_buffer:
                recon = transform.transform_kspace_to_image(c[1],dim=(1,2))*np.sqrt(scale)
                recon = np.squeeze(np.sum(recon * self.unmix,0))
                self.put_next(c[0], recon,*args)

    return 0

    if self.unmix is None:
        raise Exception("We should never reach this point without unmixing coefficients")

    recon = transform.transform_kspace_to_image(self.buffer,dim=(1,2))*np.sqrt(scale)
    recon = np.squeeze(np.sum(recon * self.unmix,0))
    self.buffer[:] = 0
    self.samp_mask[:] = 0
    self.put_next(img_head,recon,*args)

return 0

```

BUFFERING

BUFFERING

CALIBRATION

RECON

Running the Python reconstruction

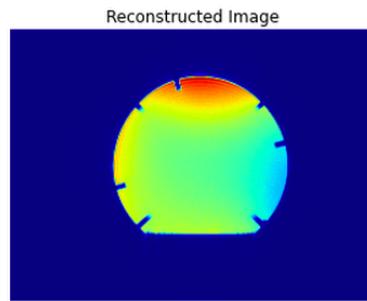
```
# Send in data
#First ISMRMRD XML header
gadget_chain_config(g_python,dset.read_xml_header())

# Loop through the rest of the acquisitions and stuff
for acqnum in range(0,dset.number_of_acquisitions()):
    acq = dset.read_acquisition(acqnum)
    g_python.process(acq.getHead(),acq.data.astype('complex64'))

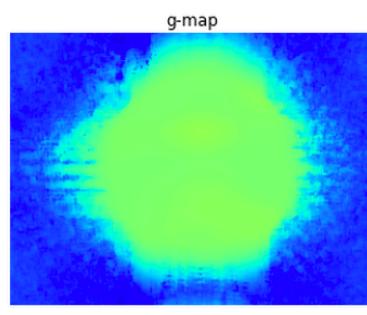
# Wait for recon to finish
gadget_chain_wait(g_python)
```

```
res_python = get_last_gadget(g_python).get_results()
gmap = get_last_gadget(g_python).gmap
```

```
show.imshow(abs(np.squeeze(res_python[0][1])),colorbar=True,titles=[ 'Reconstructed Image' ])
```



```
show.imshow(abs(np.squeeze(gmap)),colorbar=True,scale=(0,2.0),titles=[ 'g-map' ])
```



Open Source Reconstruction Frameworks

Gadgetron

COMPUTER
PROCESSING AND
MODELING -
Full Papers

Magnetic Resonance in Medicine 69:1768–1776 (2013)

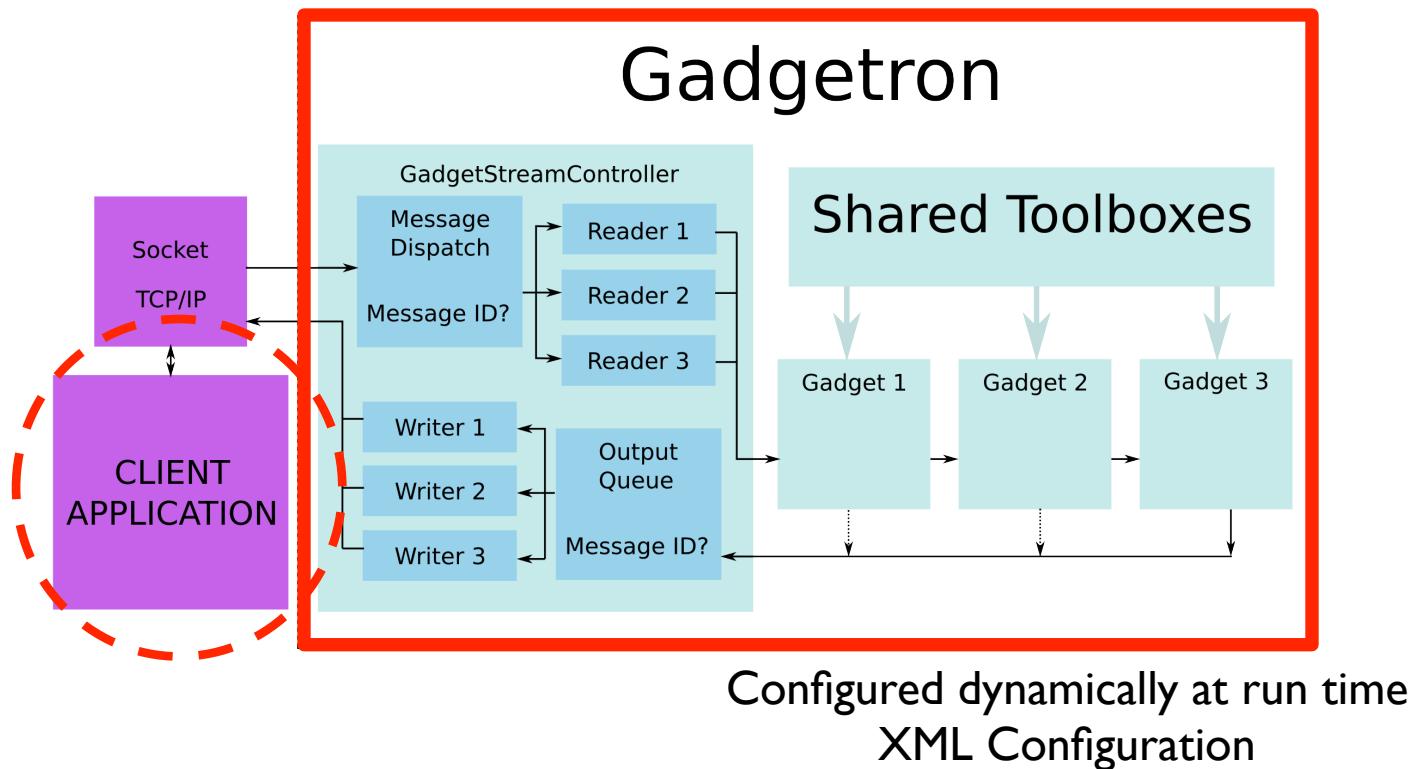
Gadgetron: An Open Source Framework for Medical Image Reconstruction

Michael Schacht Hansen^{1*} and Thomas Sangild Sørensen^{2,3}

This work presents a new open source framework for medical image reconstruction called the “Gadgetron.” The framework implements a flexible system for creating streaming data processing pipelines where data pass through a series of modules or “Gadgets” from raw data to reconstructed images. The data processing pipeline is configured dynamically at run-time based on an extensible markup language configuration description. The framework promotes reuse and sharing of reconstruction modules and new Gadgets can be added to the Gadgetron framework

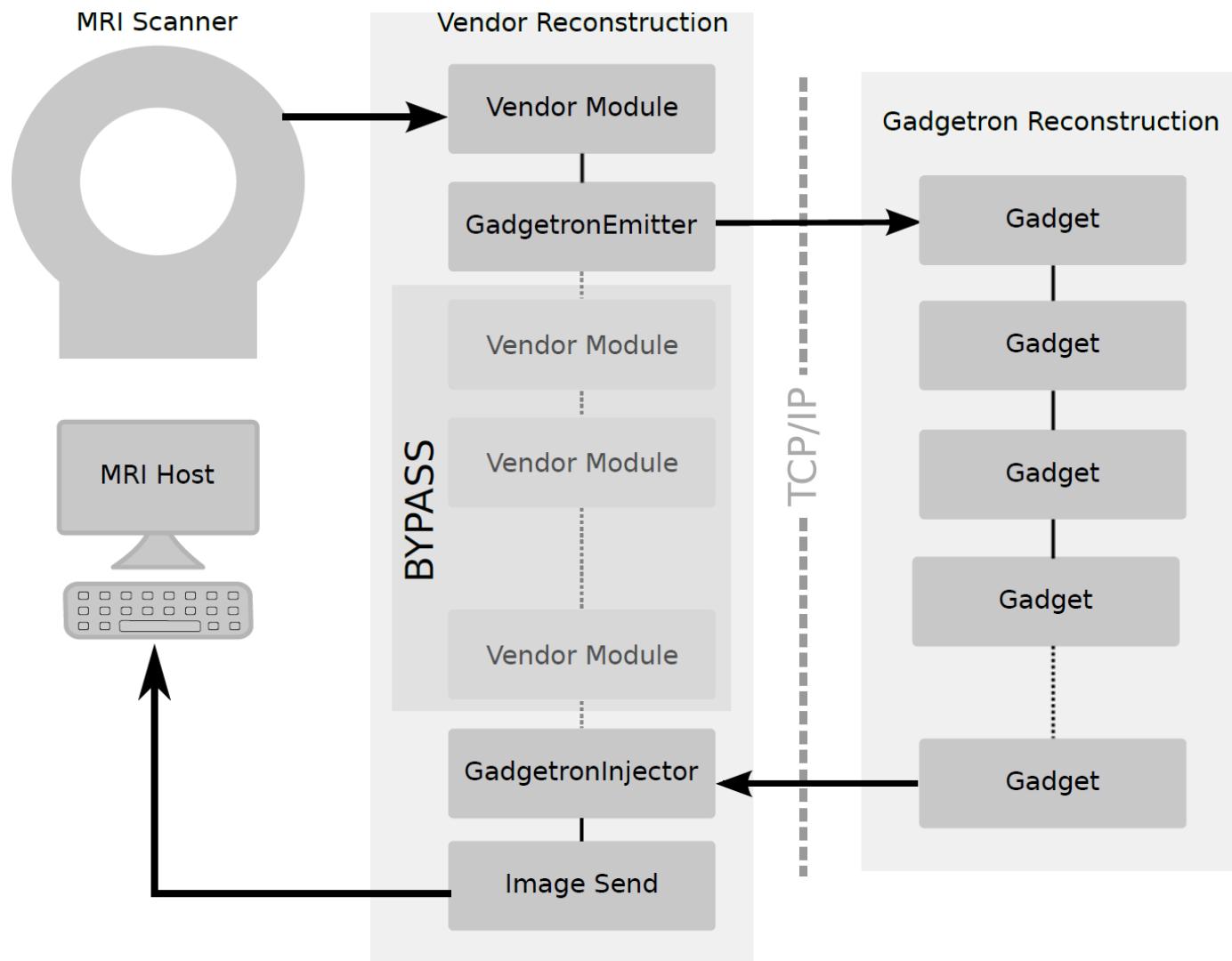
way of sharing the algorithms; they may rely on a great deal of accessory code, some of which could be vendor specific or even contain vendor-provided code that cannot be shared. Regardless of the reasons, it undermines the scientific process that readers and reviewers are prevented from reproducing the results of reconstruction research articles. It is exceedingly difficult for other researchers to evaluate how a given algorithm might perform given a different type of data or how it might interact with other algorithms. As a

Gadgetron Architecture

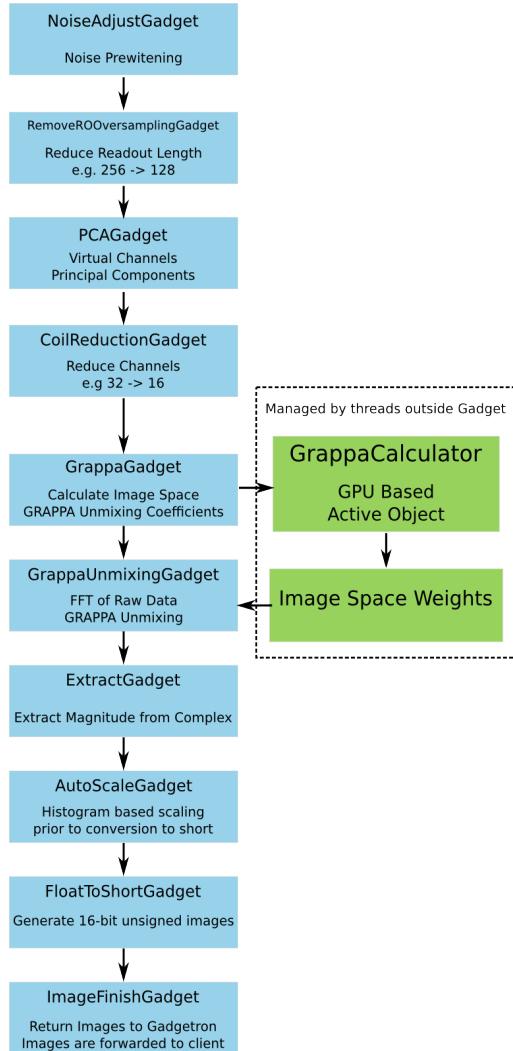


Scanner Reconstruction

Generic Scanner Integration

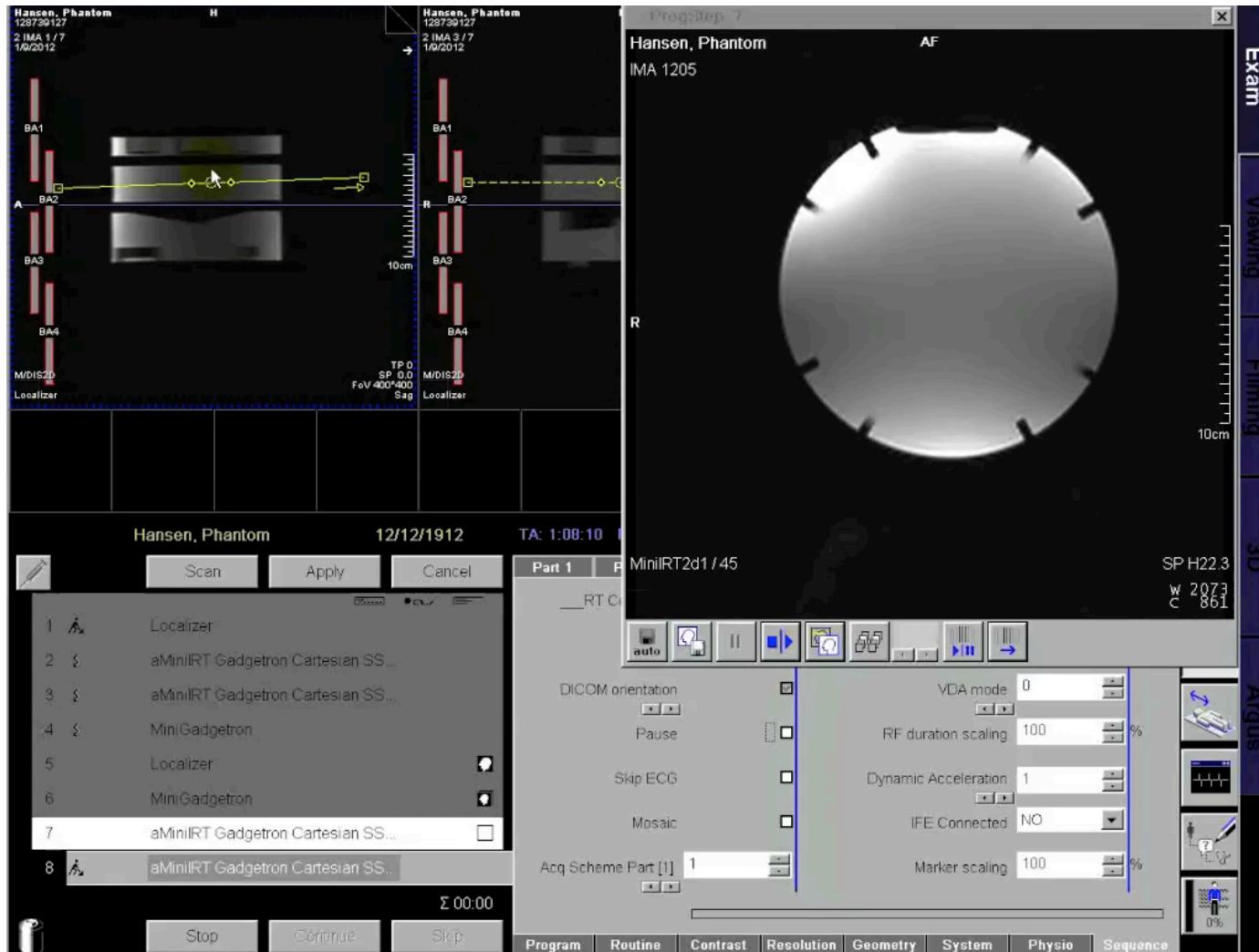


Example - Cartesian GRAPPA

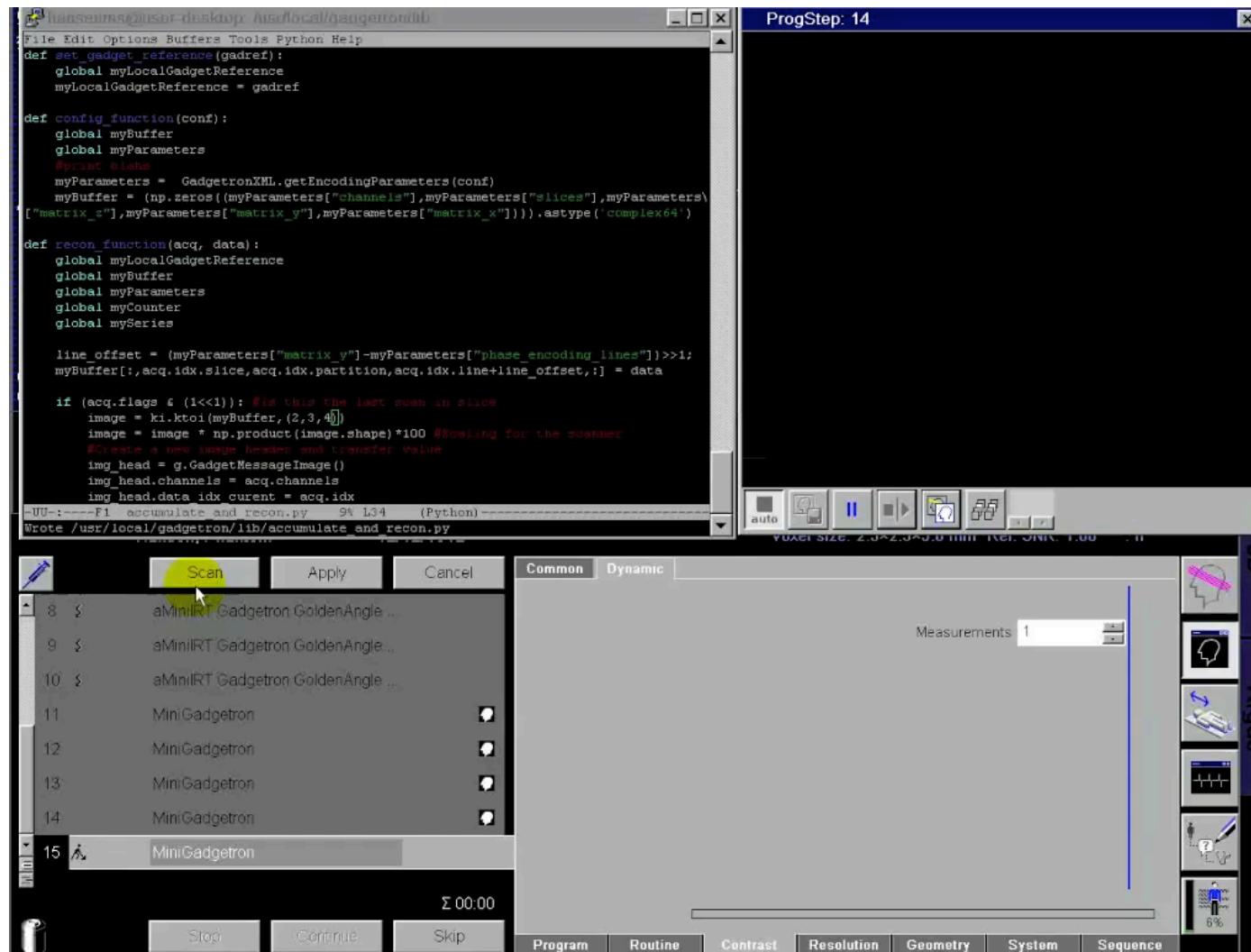


- High-throughput GRAPPA
- Designed for multi-slice 2D real-time imaging (interventional)
- GRAPPA coefficients calculated on GPU

Cartesian GRAPPA



Online Python Editing



Converting Python chains to Gadgetron

```
import gadgetron_python_to_xml as p2x
import gadgetron_xml_to_python as x2p

def define_gadget_chain():
    g2 = Recon()
    g1 = RemOS(next_gadget=g2)
    g0 = CoilReduce(next_gadget=g1)
    gb = PCA(next_gadget=g0)
    ga = NoiseAdj(next_gadget=gb)
    return ga

g_python = define_gadget_chain()

print p2x.convert_to_xml(g_python)

<?xml version="1.0" encoding="UTF-8"?>
<gadgetronStreamConfiguration xsi:schemaLocation="http://gadgetron.sf.net/gadgetron gadgetron.xsd" xmlns="http://gad
getron.sf.net/gadgetron" xmlns:xsi="http://www.w3.org/2001/XMLSchema-instance">
<reader>
    <slot>1008</slot>
    <dll>gadgetron_mricore</dll>
    <classname>GadgetIsmrmrdAcquisitionMessageReader</classname>
</reader>

<writer>
    <slot>1009</slot>
    <dll>gadgetron_mricore</dll>
    <classname>GadgetIsmrmrdAcquisitionMessageWriter</classname>
</writer>
```

Converting Gadgetron XML to Python

```
print x2p.convert_xml(os.environ['GADGETRON_HOME'] + '/share/gadgetron/config/default.xml')

# Automatically generated Python representation of /home/hansenms/local/share/gadgetron/config/default.xml

from gadgetron import WrapperGadget

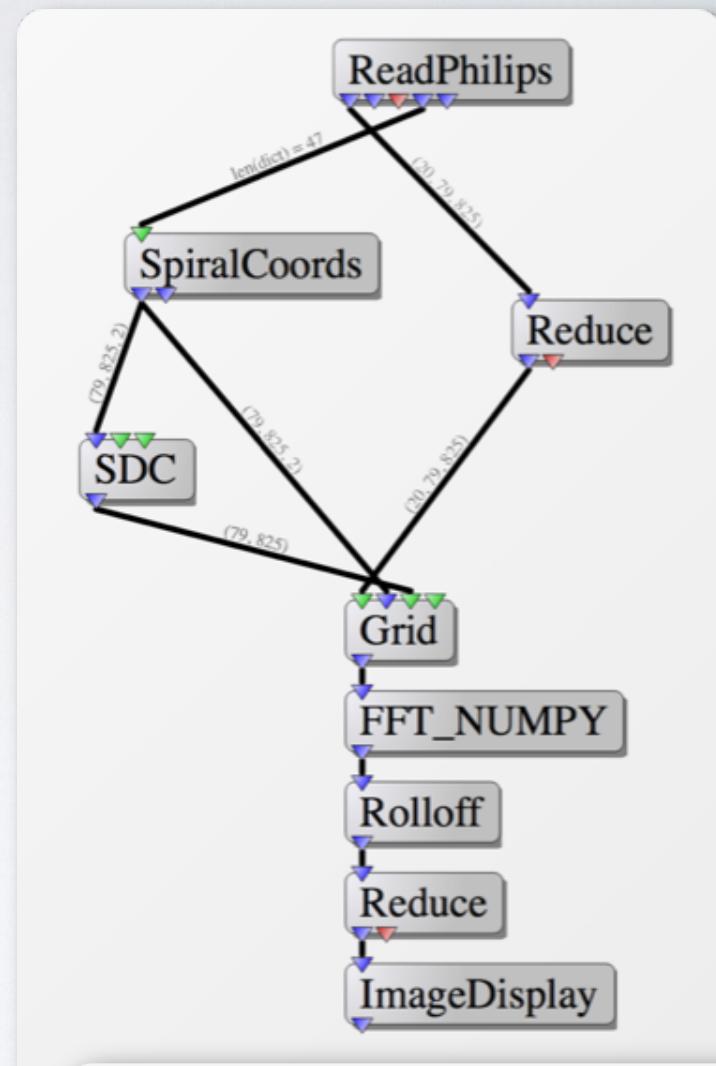
def define_gadget_chain():
    g2 = WrapperGadget("gadgetron_mricore", "ImageFinishGadget", gadgetname="ImageFinish", next_gadget=None)
    g2.prepend_gadget("gadgetron_mricore", "ExtractGadget", gadgetname="Extract")
    g2.prepend_gadget("gadgetron_mricore", "ImageArraySplitGadget", gadgetname="ImageArraySplit")
    g2.prepend_gadget("gadgetron_mricore", "SimpleReconGadget", gadgetname="SimpleRecon")
    g2.prepend_gadget("gadgetron_mricore", "BucketToBufferGadget", gadgetname="Buff")
    g2.set_parameter("Buff", "N_dimension", "")
    g2.set_parameter("Buff", "S_dimension", "")
    g2.set_parameter("Buff", "split_slices", "true")
    g2.prepend_gadget("gadgetron_mricore", "AcquisitionAccumulateTriggerGadget", gadgetname="AccTrig")
    g2.set_parameter("AccTrig", "trigger_dimension", "repetition")
    g2.set_parameter("AccTrig", "sorting_dimension", "slice")
    g2.prepend_gadget("gadgetron_mricore", "RemoveROOversamplingGadget", gadgetname="RemoveROOversampling")
    return g2
```

GPI

A Graphical Development Environment for Scientific Algorithms

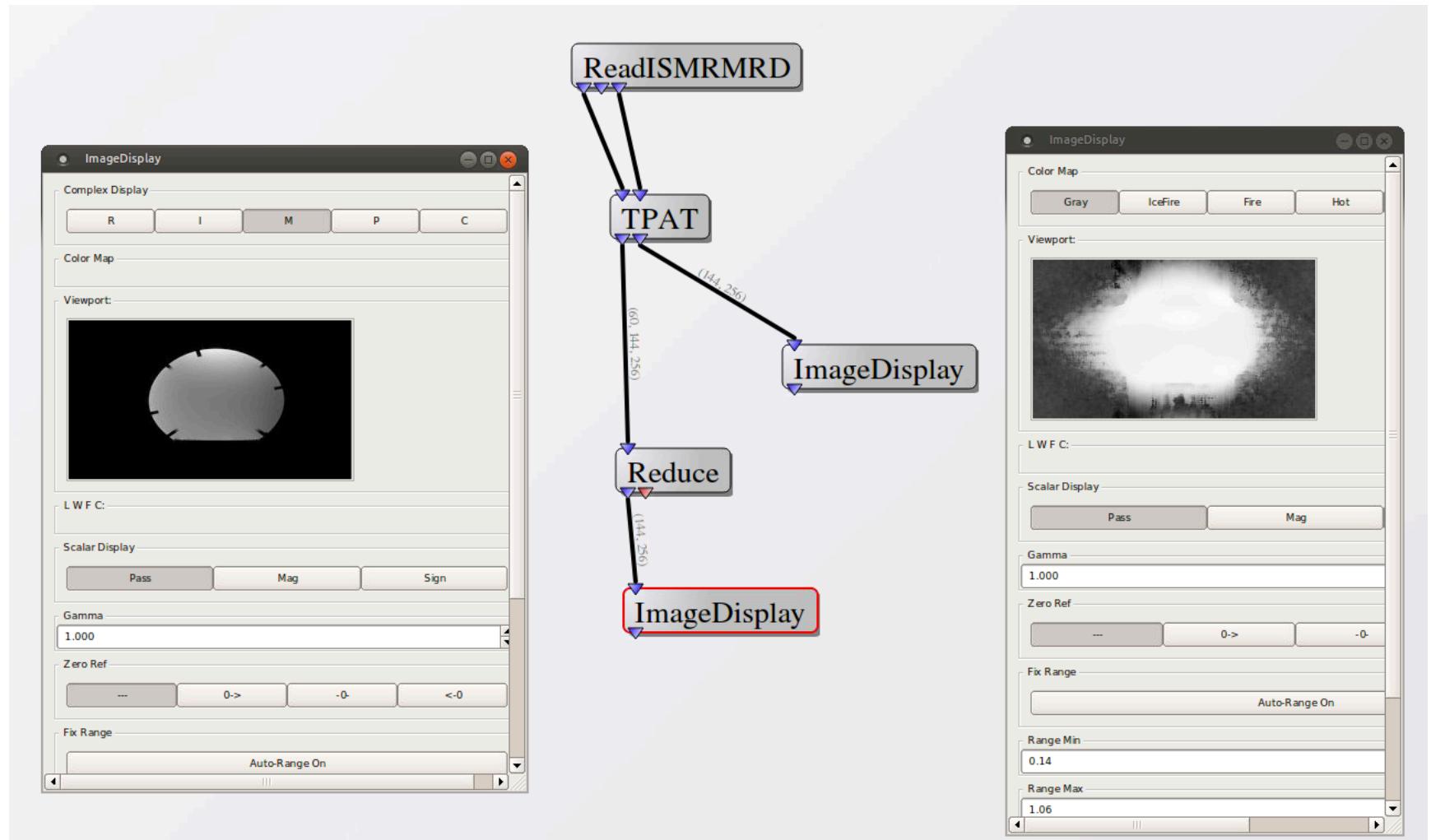
Introduction

- Modular
 - Side by Side Comparisons
 - Ease of Reuse
 - Data & Algorithm Analysis
- Reconstruction, Simulations, Pulse Sequence Development



Spiral Reconstruction

ISMRMRD Support in GPI



https://github.com/hansenms/gpi_ismrmrd

Running the Python reconstruction

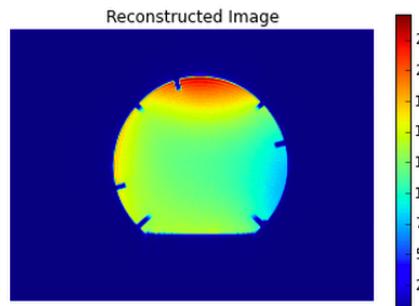
```
# Send in data
#First ISMRMRD XML header
gadget_chain_config(g_python,dset.read_xml_header())

# Loop through the rest of the acquisitions and stuff
for acqnum in range(0,dset.number_of_acquisitions()):
    acq = dset.read_acquisition(acqnum)
    g_python.process(acq.getHead(),acq.data.astype('complex64'))

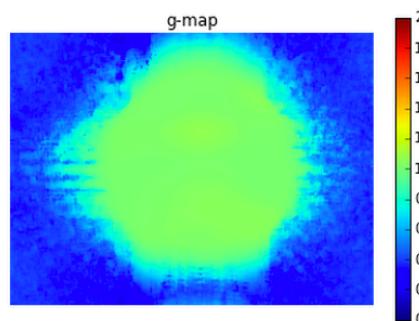
# Wait for recon to finish
gadget_chain_wait(g_python)
```

```
res_python = get_last_gadget(g_python).get_results()
gmap = get_last_gadget(g_python).gmap
```

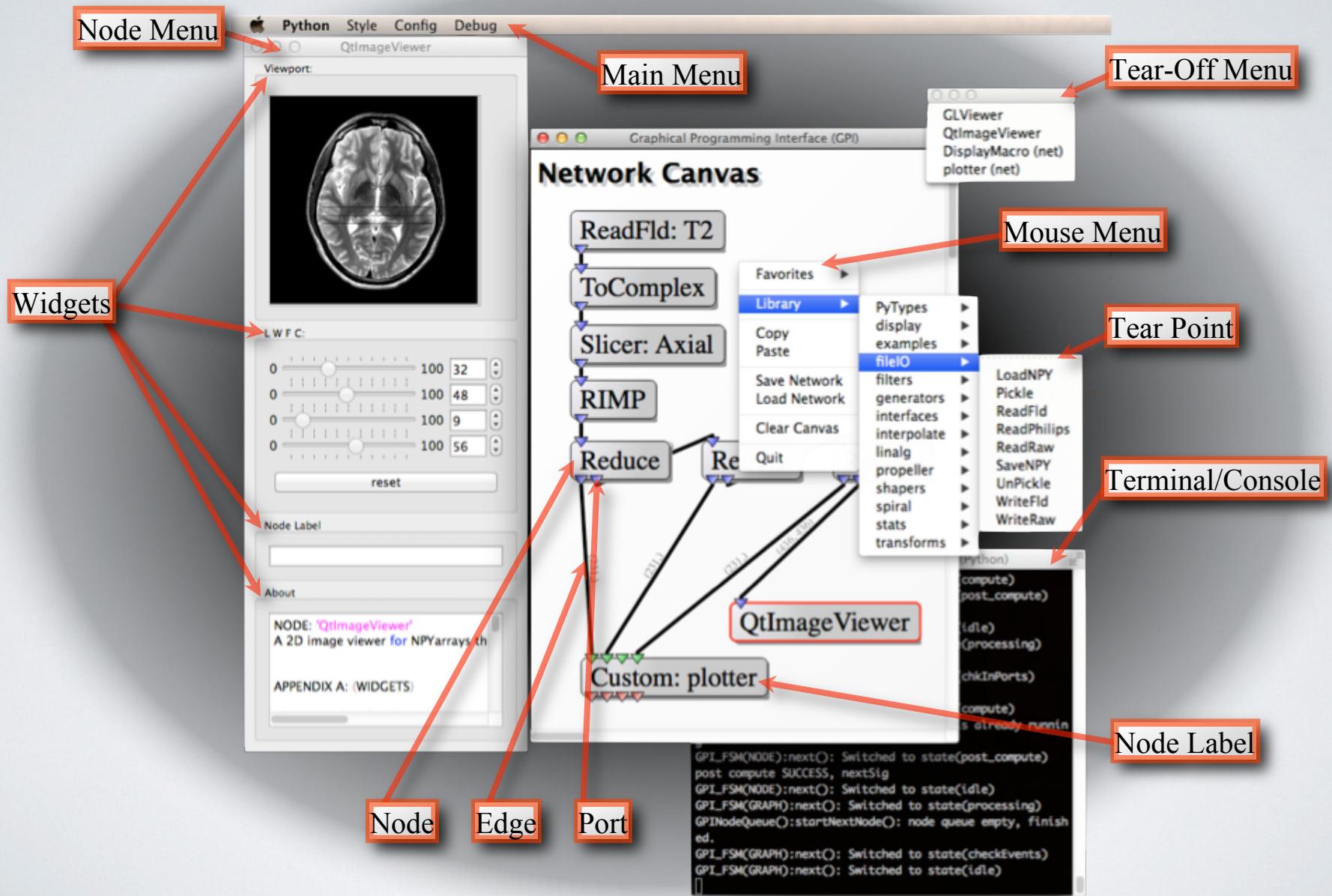
```
show.imshow(abs(np.squeeze(res_python[0][1])),colorbar=True,titles=[ 'Reconstructed Image' ])
```



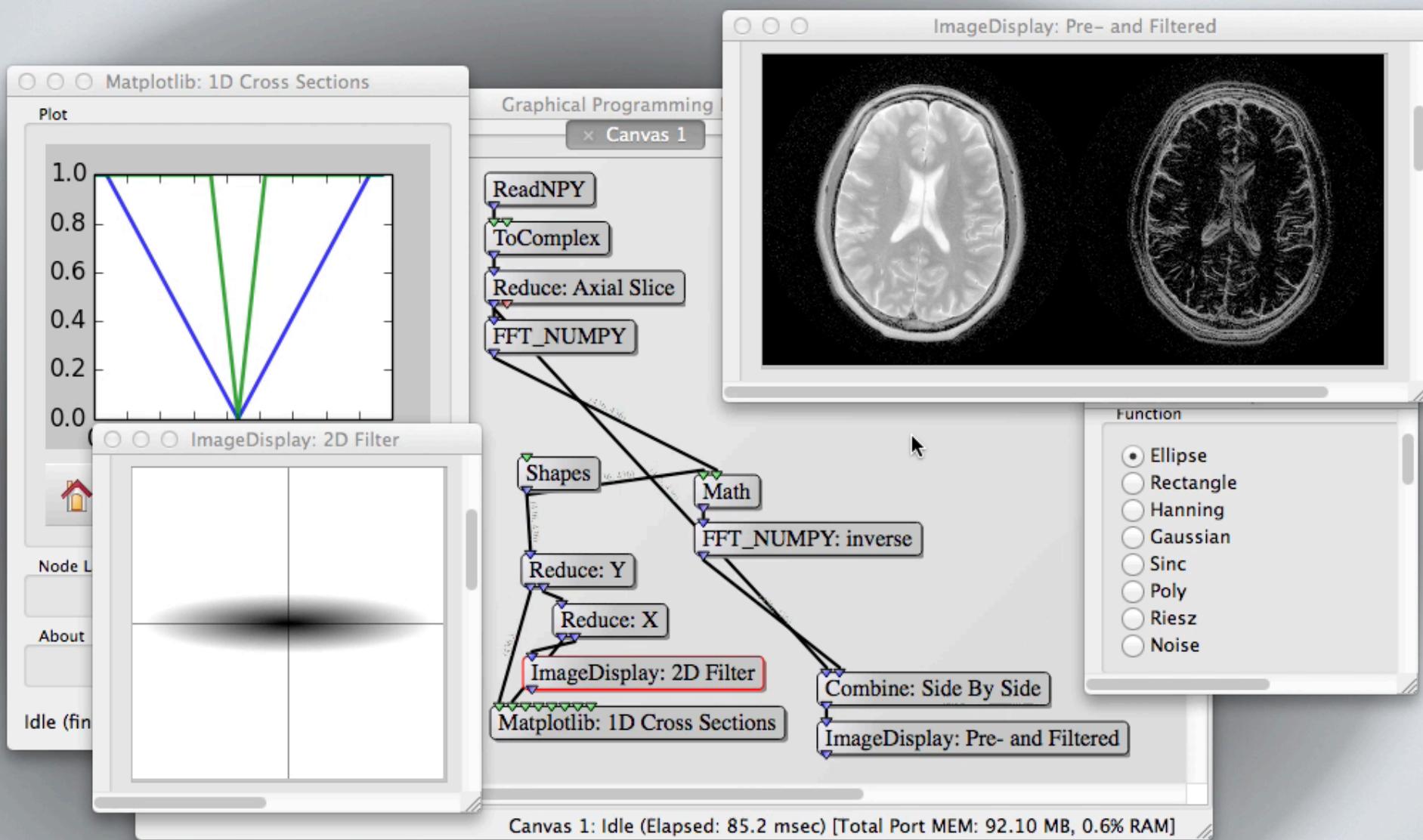
```
show.imshow(abs(np.squeeze(gmap)),colorbar=True,scale=(0,2.0),titles=[ 'g-map' ])
```



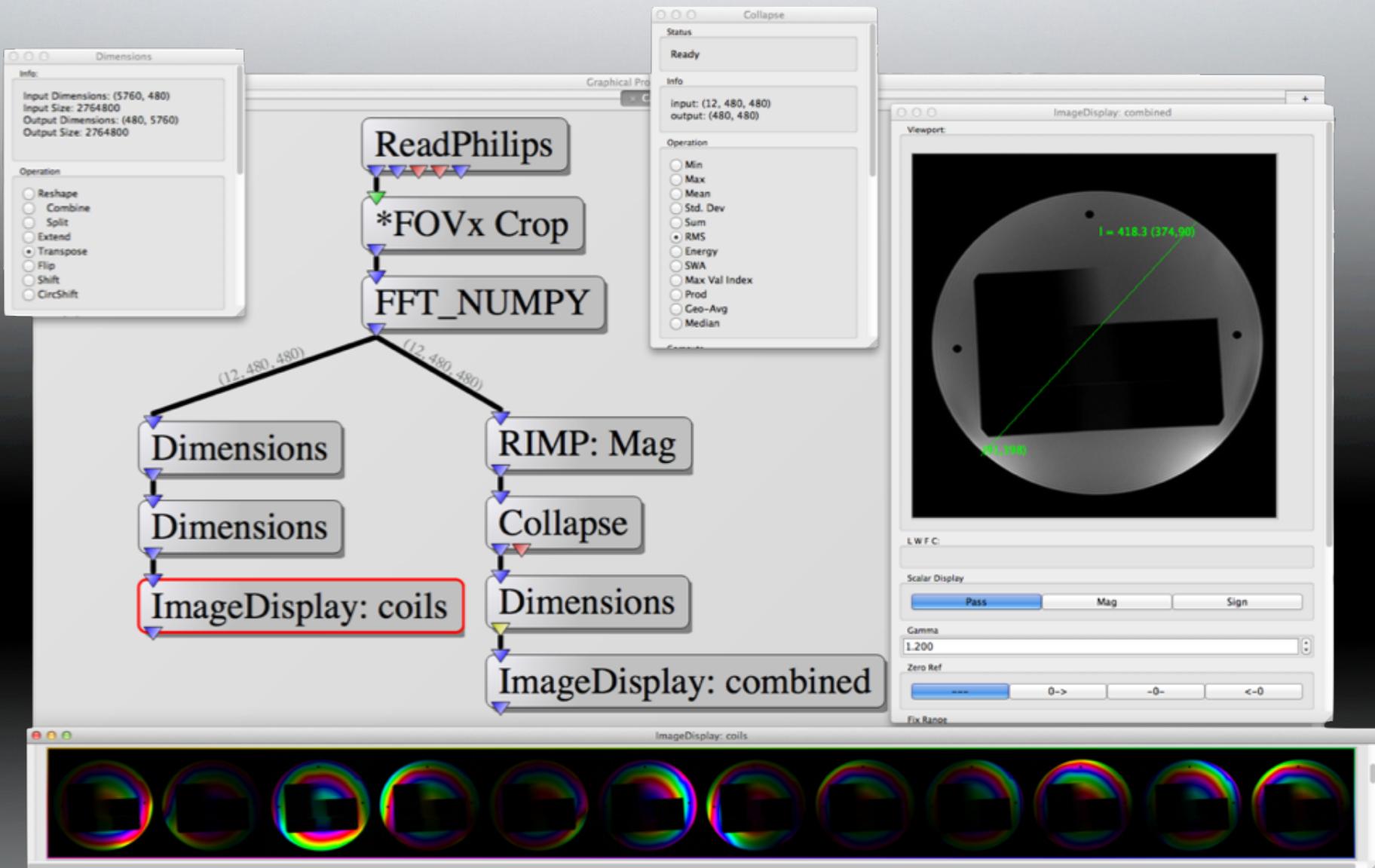
Graphical interface



K-space filter



coil combination



codeare

Common Data Exchange And Reconstruction
www.codeare.org

Realisation

Algorithm library and client/server application

- N-dimensional Data structure called “**Matrix**”
- **Algorithm dictionary** for arithmetic, linear algebra, Fourier transformation, statistics, optimisation, file IO, ...
- Near **textbook high level language** for implementation

```
Matrix<cf> A = phantom<cf>(256), B,  
        cxnoise = randn<cf>(256);  
  
DFT<f> F;  
B = F / (F*A + cxnoise);  
print (B, 'B.png', 'r600');  
fopen (f, 'B.mat', WRITE);  
fwrite (f, conj(B));  
fclose (f);
```

- Usage
 - C++ library
 - stand alone application
 - client server application for realtime scanner feedback

Usage

Reconstruction chain

- Reconstruction strategies often involve multiple reusable steps
- Example on write is part of the package to demonstrate how this is achieved in codeare
- Real-day example involves the estimation of receive sensitivities, reduction of coils and subsequent CS reconstruction

```
<?xml version="1.0" ?>
<config paradigm="SHM">

  <!-- R=6.0 coherent(3.0) * incoherent(2.0)
      Variable density spiral @ 3T -->
  <data-in fname="cgssense_r3_cs.h5" ftype="HDF5">
    <kspace uri="kspace" dtype="float"/>    <!-- trajectory -->
    <weights uri="weights" dtype="float"/>  <!-- weights -->
    <!-- Phase correction -->
    <phase_correction uri="phase_correction" dtype="cxfl"/>
  </data-in>

  <!-- Reconstruction chain -->
  <chain>
    <!-- Estimate sensitivities
        Reconstruct channels with NuFFT
        Constraint smoothing with LBFGS -->
    <EstimateSensitivities dim="2" Nx="192" Ny="192" maxit="1"
                           epsilon="2.0e-2" m="1" alpha="1.0"
                           verbose="1" M="9600" shots="8"
                           optimiser="LBFGS"/>

    <!-- Reduce channels -->
    <ReduceReceiveChannels dim="2" threshold="7.5e-3"/>

    <!-- Non Cartesian accelerated CS
        ft="3": Non-Cartesian SENSE
        Constraint optimisation: Split-Bregman -->
    <CompressedSensing ft="3" ftmaxit="2" fsteps="7.0e-4" cgmaxit="2"
                        cgeps="1.0e-5" verbose="1" noise="1.5"
                        ftdims="192,192" lambda="1.0e-8" threads="8"
                        csiter="5" tvw="5.0e-3" xfmw="5.0e-4"
                        cgiter="4" cgconv="1.0e-3" l1="1.0e-8"
                        lsiter="30" pnorm="1.0" lslim="10" lsa="0.01"
                        lsb="0.5" lsto="1" wl_family="0" wl_member="4"
                        image_size="256" test_case="1" nk="13758"
                        optimiser="SplitBregman"/>

  </chain>

  <!-- Output -->
  <data-out ftype="HDF5" fname="csout.h5">
    <res uri="res" dtype="cxfl"/>
    <sensitivities uri="sensitivities" dtype="cxfl"/>
  </data-out>

</config>
```

Critical Components of Pipeline Processing

- Modularity
 - Reusable code
- Event driven processing
- Multi-threading
- Standardized raw data representation
 - Meaningful data labels

THANK YOU

- Jeff Voskuil, GE Healthcare
- Amol Pednekar, Philips Healthcare
- Wes Gilson, Siemens Healthcare
- Nick Zwart, GPI, Barrow Neurological Institute, Phoenix AZ
- Kaveh Vahedipour, NYU
- Souheil Inati, National Institutes of Health
- Joe Naegele, National Institutes of Health
- Hui Xue, National Institutes of Health

Open Source Resources

- Course Materials: <http://hansenms.github.io/sunrise>
- ISMRMRD:
 - <http://ismrmrd.github.io>
 - <http://github.com/ismrmrd/ismrmrd-python>
 - <http://github.com/ismrmrd/ismrmrd-python-tools>
- GADGETRON:
 - <http://gadgetron.github.io>
- GPI:
 - <http://gpilab.com>
 - http://github.com/hansenms/gpi_ismrmrd
- CODEARE:
 - <http://www.codeare.org>