

Deep learning for medical image registration

Ruisheng Su

Maureen van Eijnatten

Outline for today:

- Quick recap of medical image registration
- Introduction non-parametric / deformable image registration
- Deep learning for medical image registration:
 - Deep iterative registration
 - Supervised methods
 - Unsupervised (optimization-based) methods

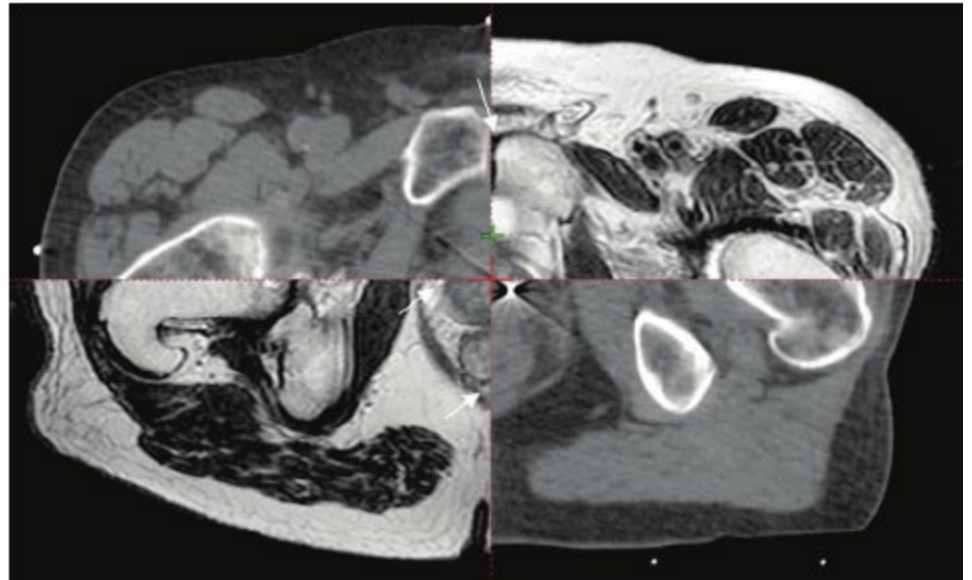
Recap: medical image registration

Why important?

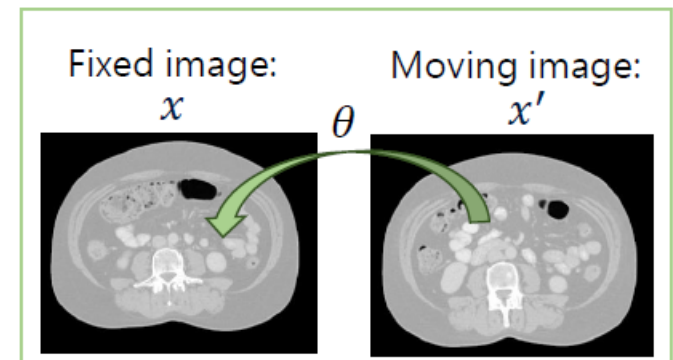
- Multi-modal registration (e.g. CT on MRI)
- Inter-subject (e.g. atlas registration)
- Longitudinal (e.g. treatment evaluation)

Remaining challenges:

- Large 3D volumes
- Accuracy vs. efficiency
- Intensity inhomogeneities and discontinuities
- Outlier rejection



Medical image registration: general “recipe”



Transformation model:
(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure:
(e.g. SSD, CC, MI, MSE)

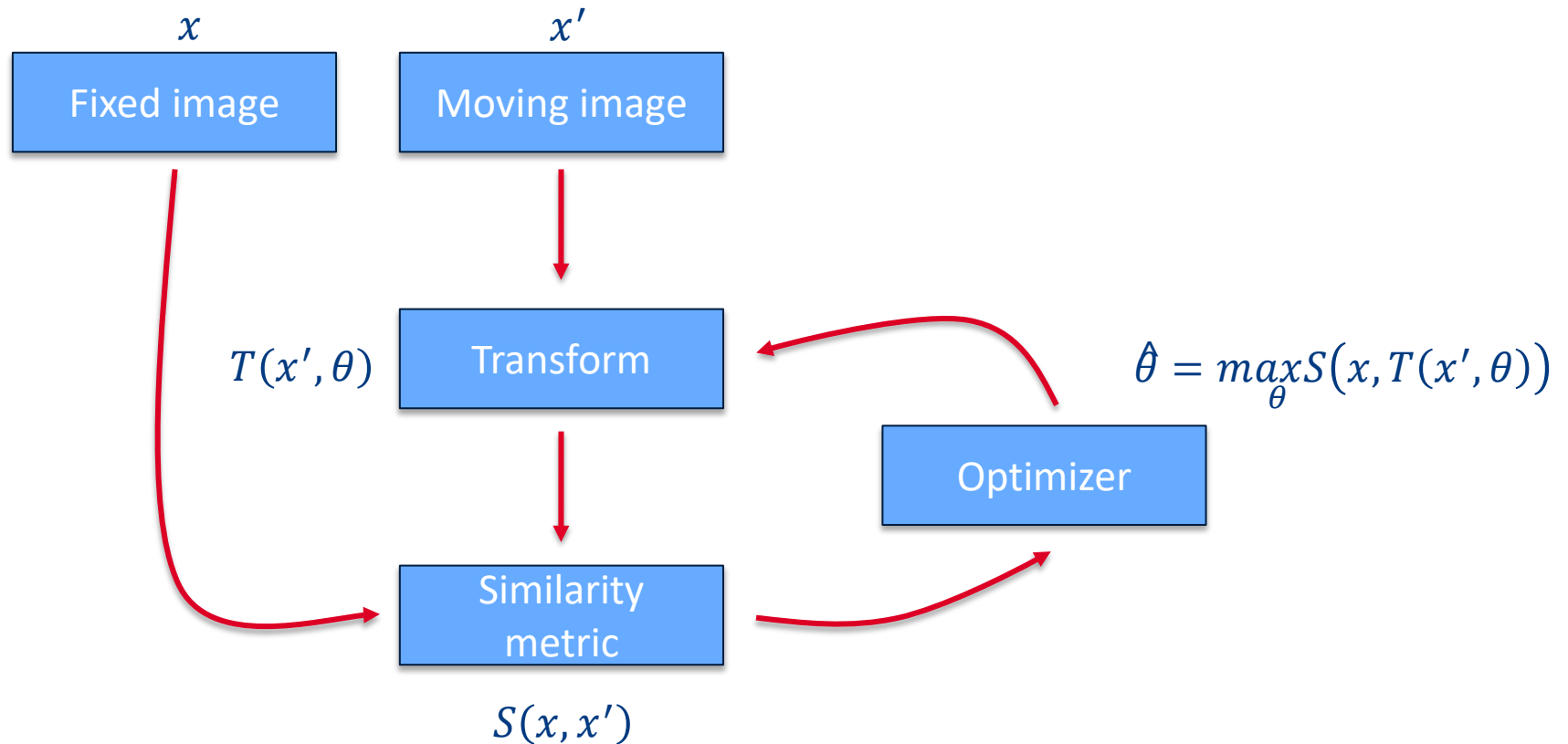
$$S(x, x')$$

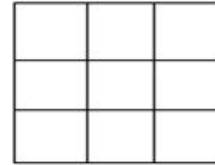
**Image
registration**

Optimization:

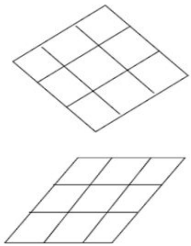
$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

Finding the optimal transformation



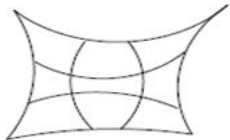


Transformation models



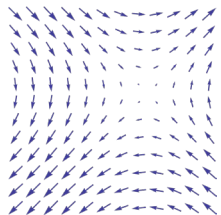
Rigid & Affine

- Point or feature-based (e.g. landmarks, fiducials)
- Intensity-based
- Gradient/edge-based



Non-linear

- Linear or higher order polynomials
- Spline-based



Non-parametric / deformable

- Allowing each image element to be displaced arbitrarily

Rigid transformations

- Translation
- Rotation

$$\mathbf{x}' = \mathbf{R}\mathbf{x} + \mathbf{t}$$

$$\mathbf{t} = \begin{bmatrix} t_x \\ t_y \end{bmatrix}$$

$$\mathbf{R} = \begin{bmatrix} \cos(\phi) & -\sin(\phi) \\ \sin(\phi) & \cos(\phi) \end{bmatrix}$$

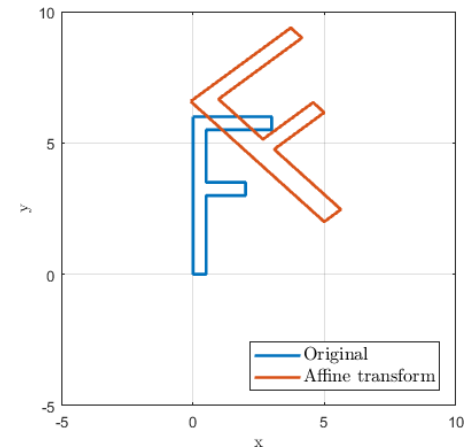
Affine transformations: translation, rotations and

- Scaling
- Shearing

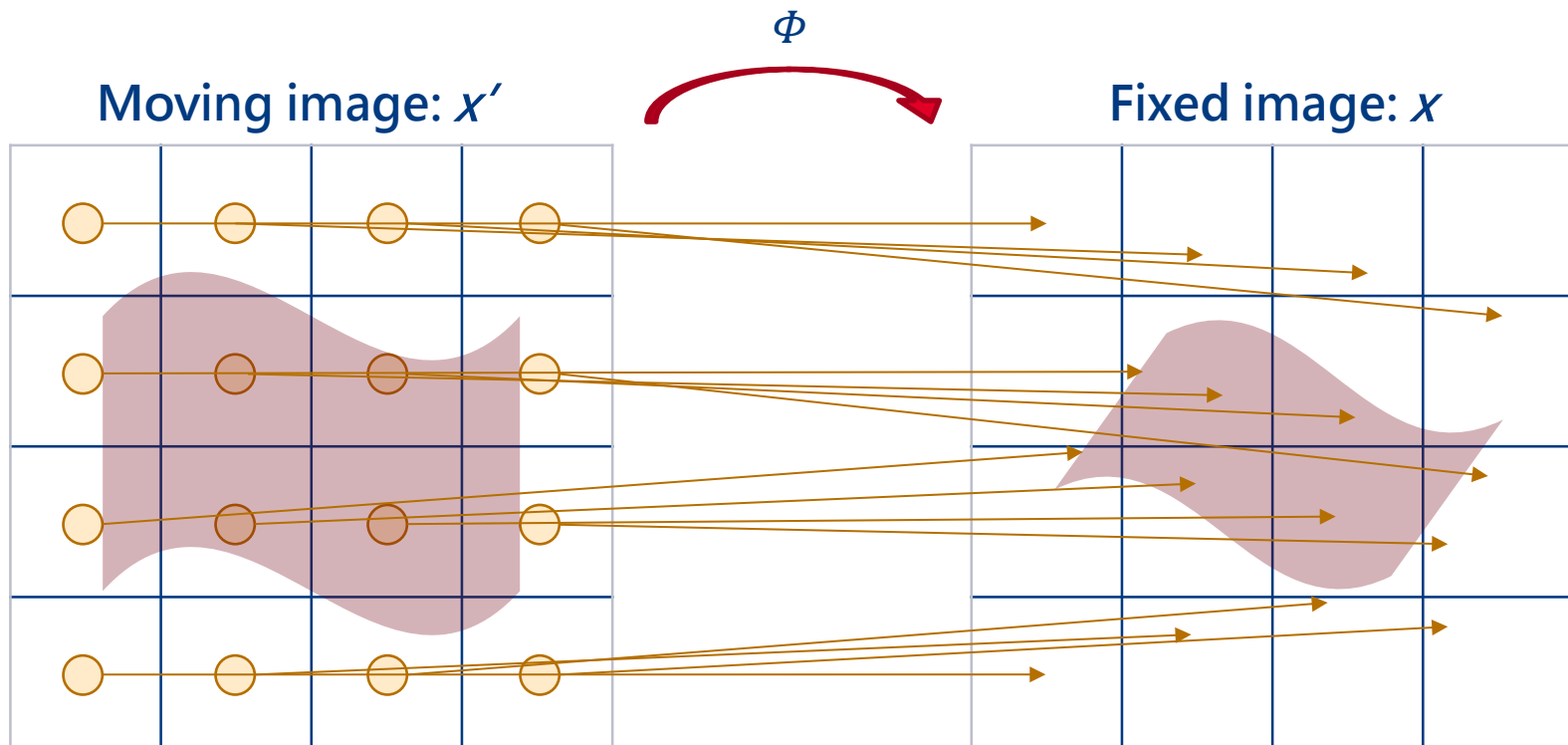
$$\mathbf{x}' = \mathbf{A}\mathbf{x} + \mathbf{t}$$

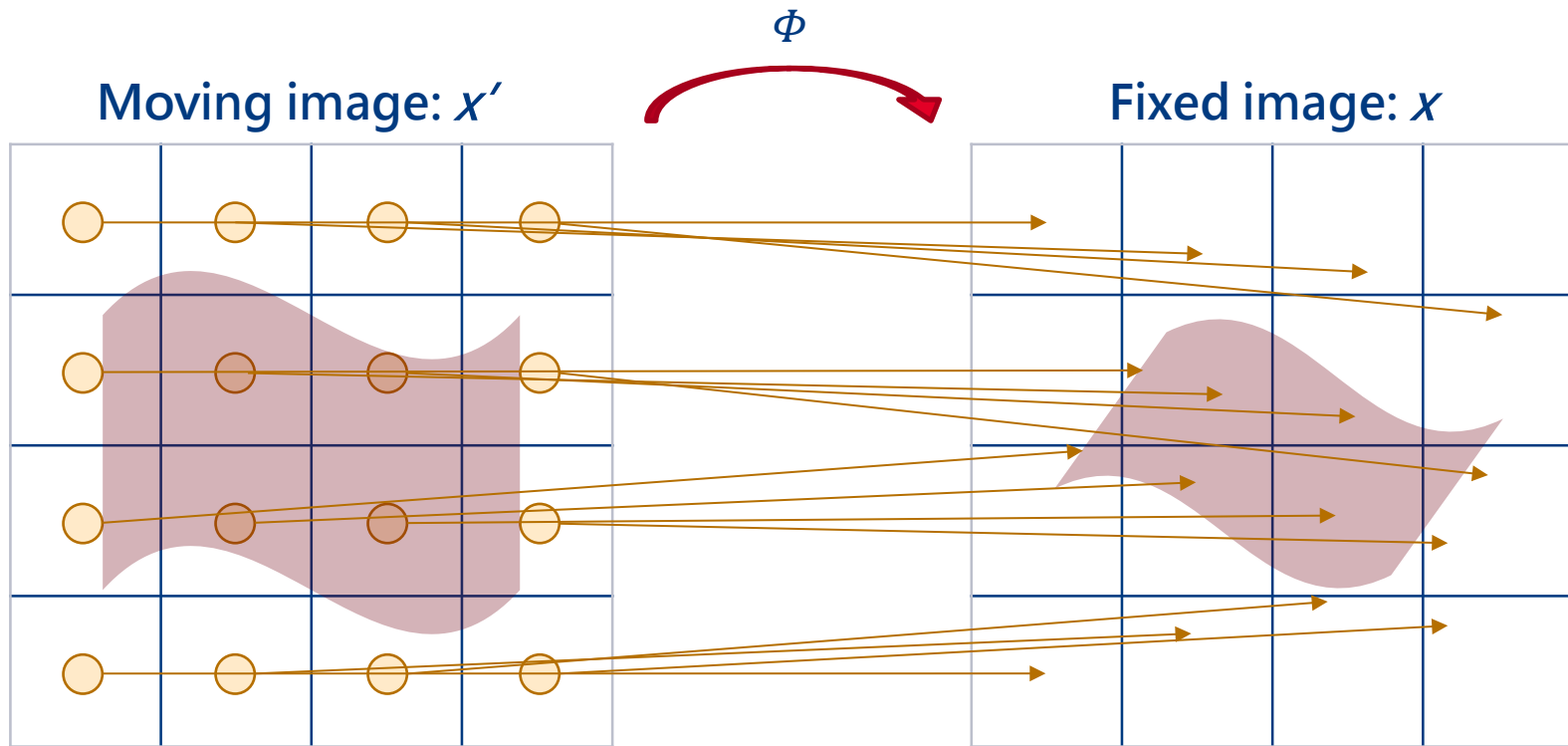
$$\mathbf{S} = \begin{bmatrix} s_x & 0 \\ 0 & s_y \end{bmatrix}$$

$$\mathbf{H} = \begin{bmatrix} 1 & h_x \\ h_y & 1 \end{bmatrix}$$



Displacement (vector) field (DVF) = Dense set of vectors representing the displacement in a given spatial domain



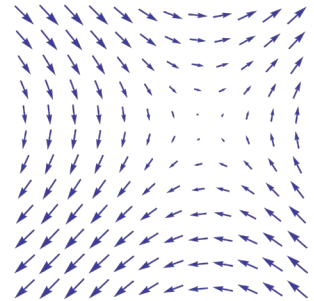


Deformation: $\varphi = Id + u, \varphi: \Omega \rightarrow \mathbb{R}^d$
 or point-wise: $\varphi(x) = x + u(x)$

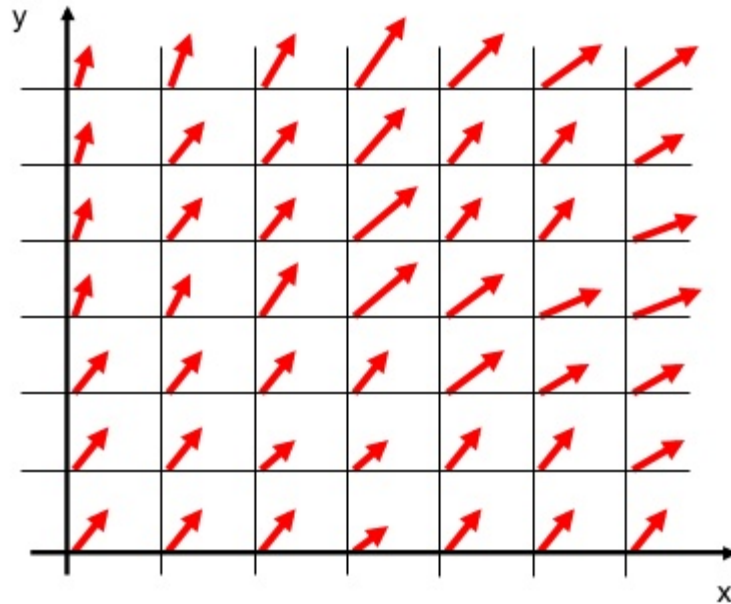
Displacement:

$$u: \Omega \rightarrow \mathbb{R}^d$$

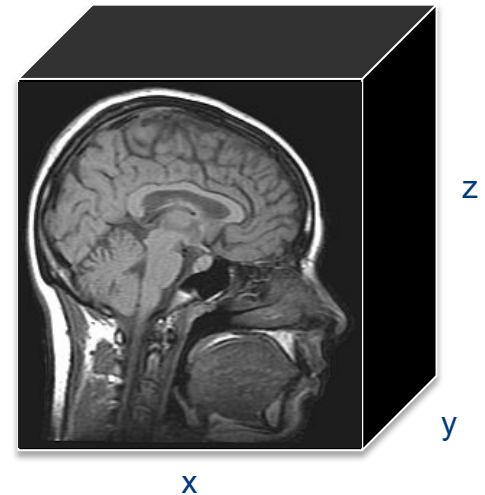
e.g. u
 $= [u_x, u_y, u_z]$



Deformable image registration: how many free parameters (DOF) in 3D?



Typical spatial resolution of a
3D medical image
(MRI: e.g. $1.5 \times 1.5 \times 4 \text{ mm}^3$ voxels)



$$\text{DOF} = 3 \cdot N_x \cdot N_y \cdot N_z (!)$$

Deformable image registration is still a very active area of research, and many different deformable registration models exist:

- Free-form deformation model
- Optical flow
- Demons
- Fluid flow
- Diffeomorphisms
- ...

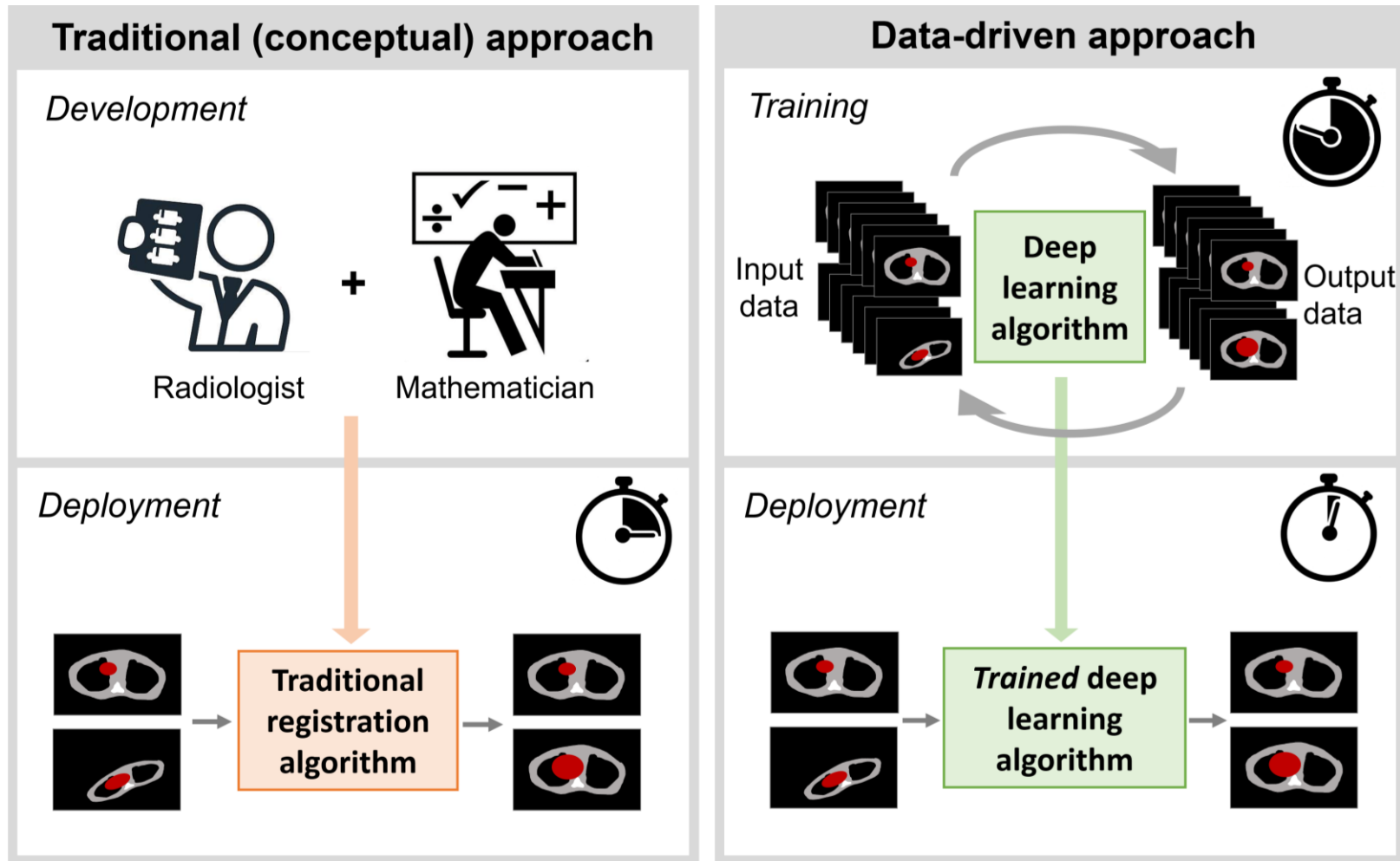
Note that the details of these models and their implementations are beyond the scope of this course.

Learning goals of this lecture

The students should be able to:

- Explain the difference between parametric and non-parametric image registration models
- Formulate deformable image registration as an optimization problem
- Understand displacement vector fields
- Explain the difference between supervised and unsupervised learning
- Understand why deep learning is an interesting technique to solve medical image registration tasks
- Understand the different ways in which deep learning can be used to perform (deformable) image registration

Why focus on deep learning for medical image registration?



Machine learning – different training strategies

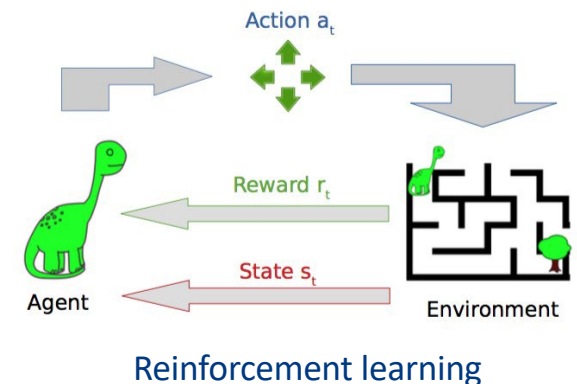
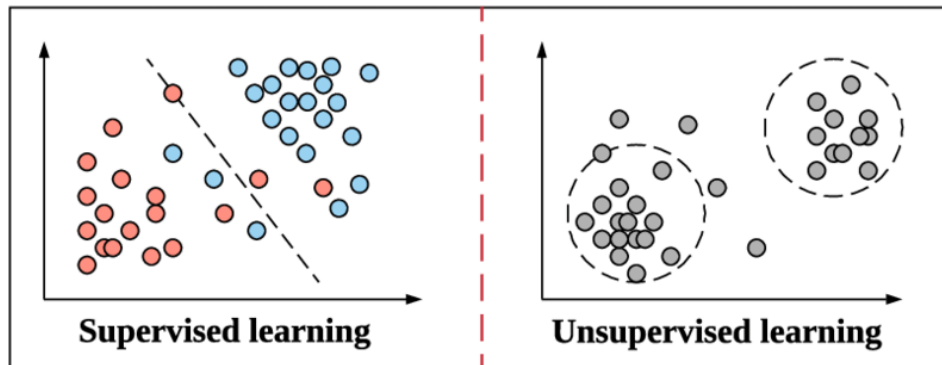
Supervised learning = develop predictive model based on input and output data (i.e., ground truth, “labels”)

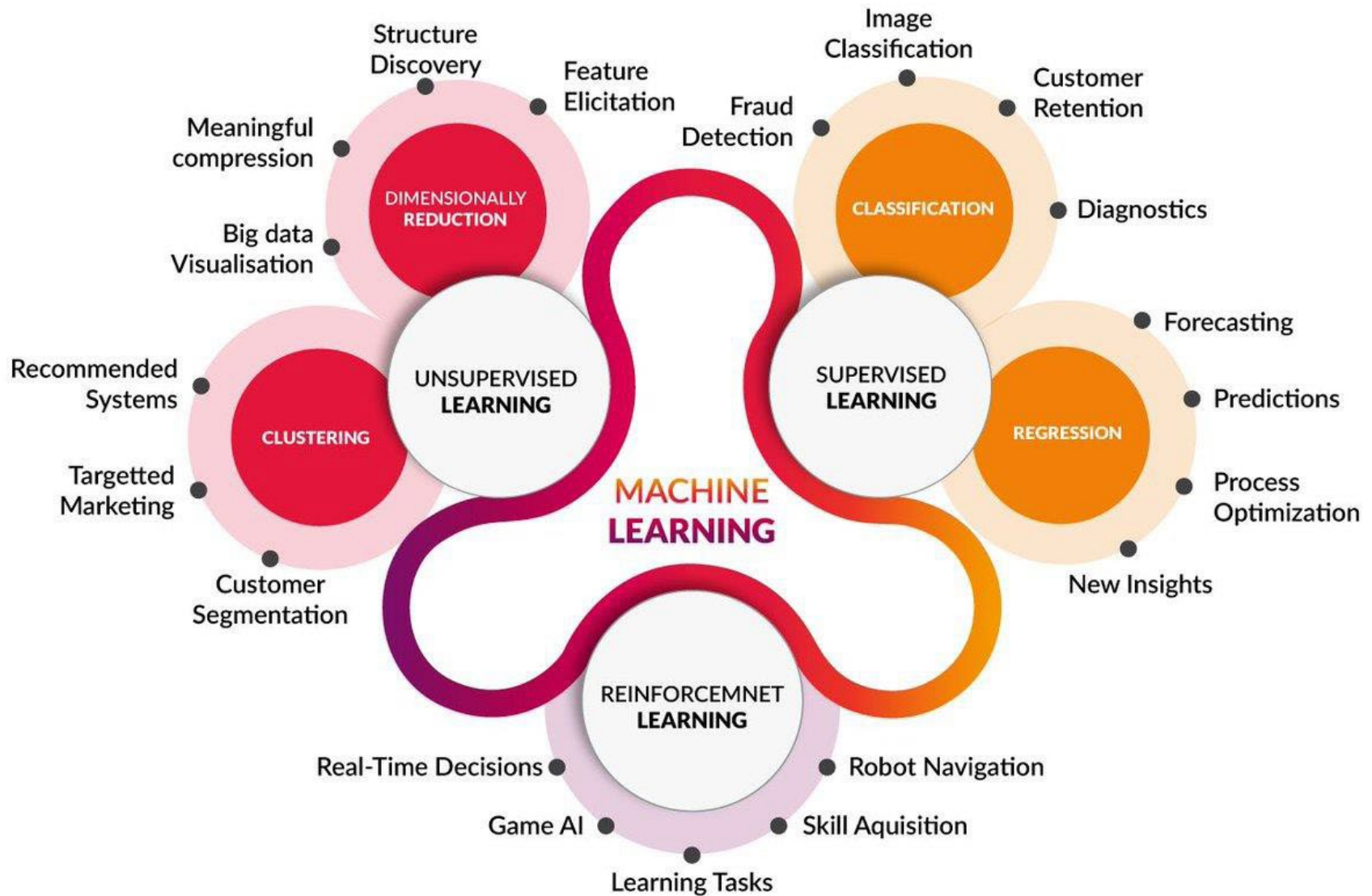
Examples: classification (e.g., skin lesion classification), regression (segmentation of vessel structures)

Unsupervised learning = group or interpret data based on input data alone

Example: clustering (e.g., k-means)

NB: also semi-supervised learning and reinforcement learning, not part of this course.





Learning image registration: how does it work?

Problem: how can we obtain the ground truth displacement ?

A. Deep iterative registration

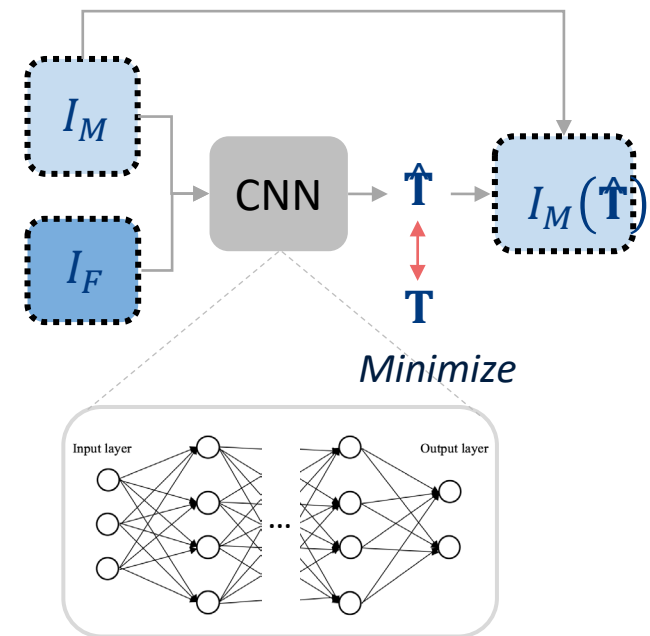
- Learn a component of a classical registration method

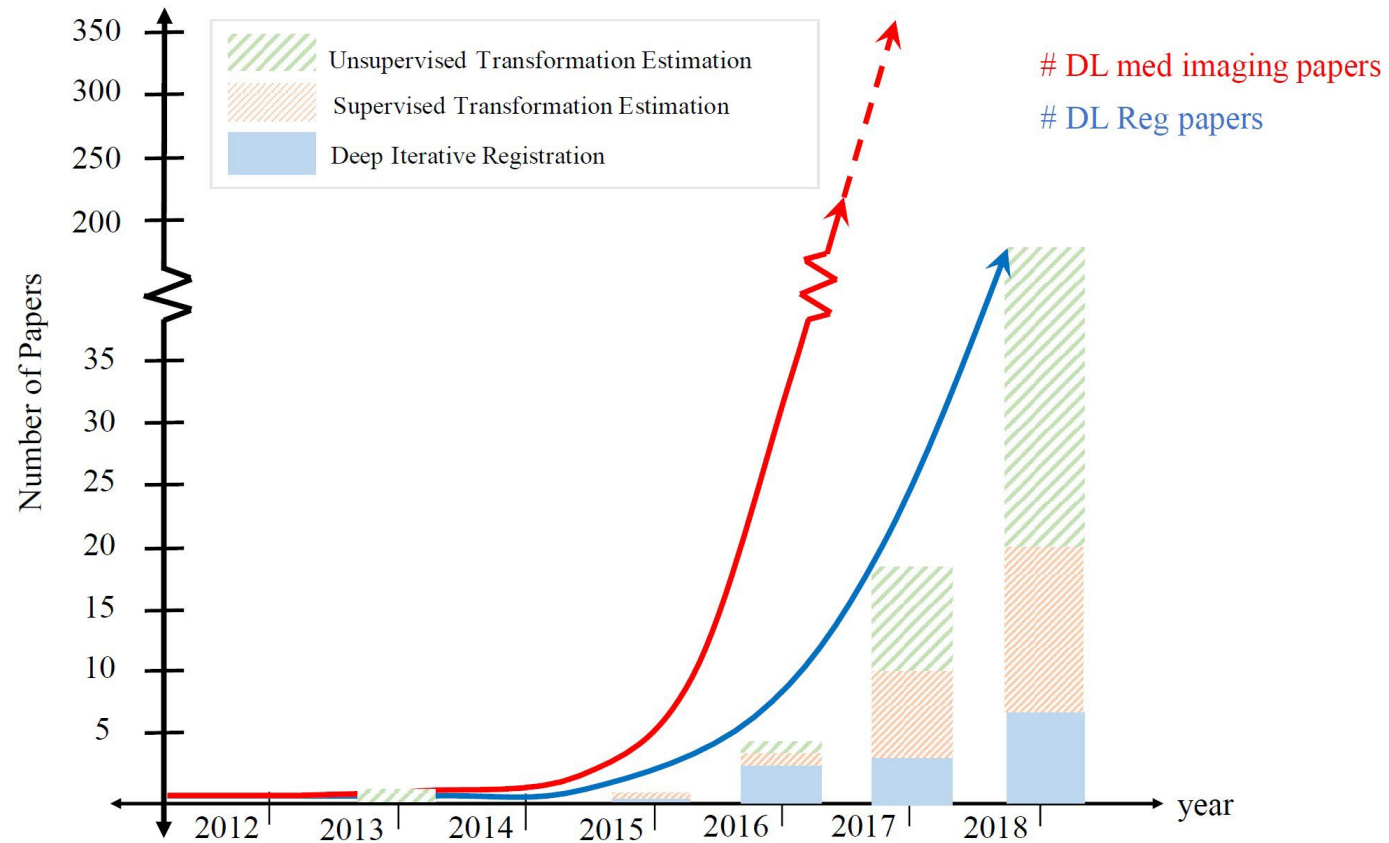
B. Supervised transformation estimation

- Obtain using classical registration method
- or make synthetic ground truth

C. Unsupervised transformation estimation

- Use similarity metric to judge





A. Deep iterative registration

Use a traditional registration method and learn one component

Automatically extract (learn) similarity features

- *Unimodal*: Wu et al. (2013) Unsupervised deep feature learning for deformable registration of mr brain images (MICCAI); Wu et al. (2016) Scalable high-performance image registration framework by unsupervised deep feature representations learning (IEEE Transactions on Biomedical Engineering); Eppenhof et al. (2018) Error estimation of deformable image registration of pulmonary ct scans using convolutional neural networks (Journal of Medical Imaging)
- *Multimodal*: Mostly *rigid registration*; learn a similarity metric to evaluate or register multimodal images using gradient descent. E.g. Cheng et al. (2016&2018) Deep similarity learning for multimodal medical images (MICCAI)

Reinforcement learning

Mostly used for *rigid registration*

- Low-resolution transformation model for deformable registration
Krebs et al. (2017) Robust non-rigid registration through agent-based action learning (MICCAI)

Where are we in the image registration “recipe”?

Transformation model:
(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure:
(e.g. SSD, CC, MI, MSE)

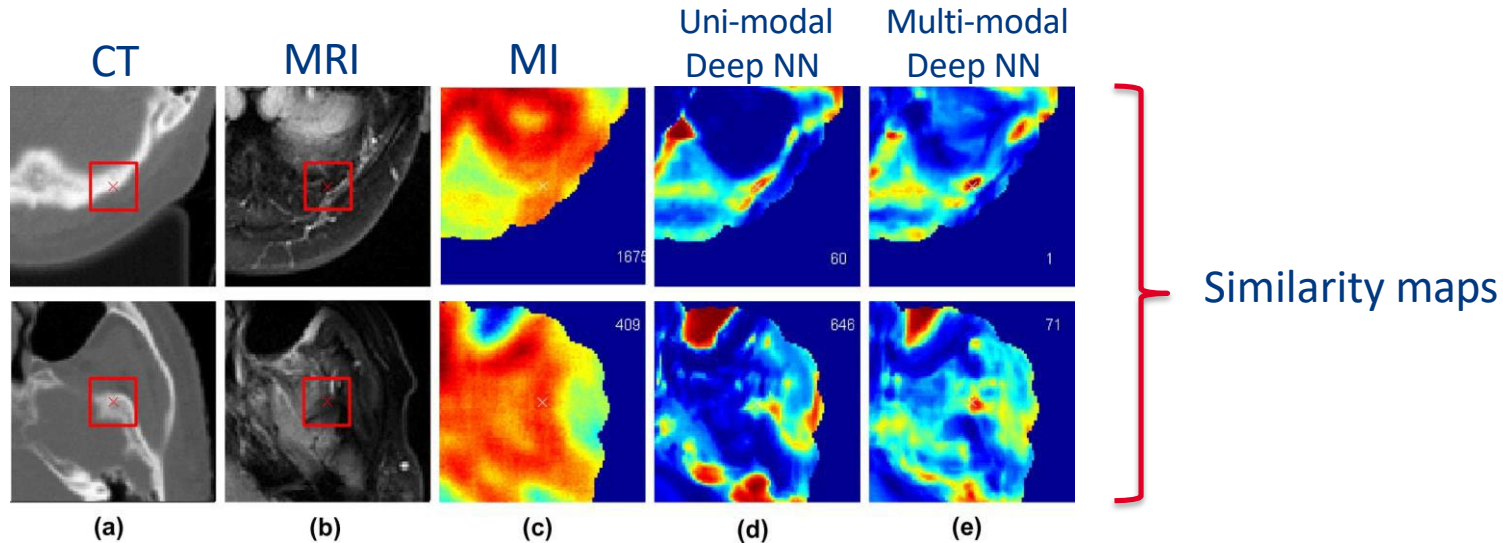
$$S(x, x')$$

Image
registration

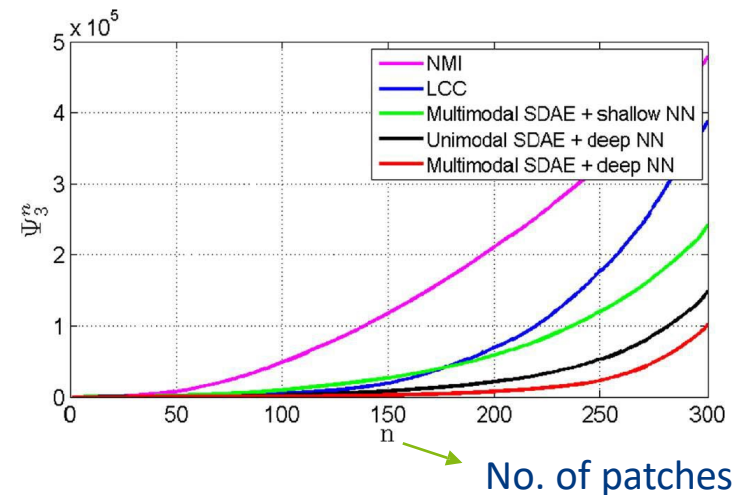
Optimization:

$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

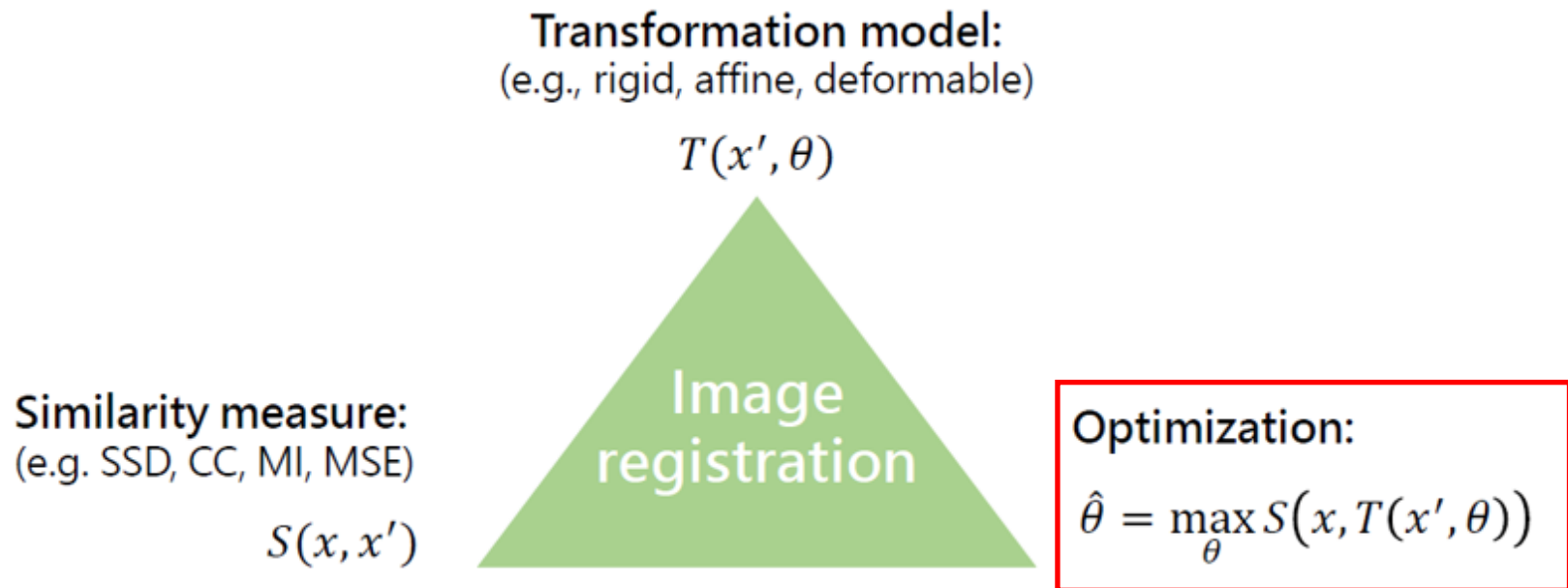
Example 1: Learning multimodal feature extraction (Haskins et al., 2019)



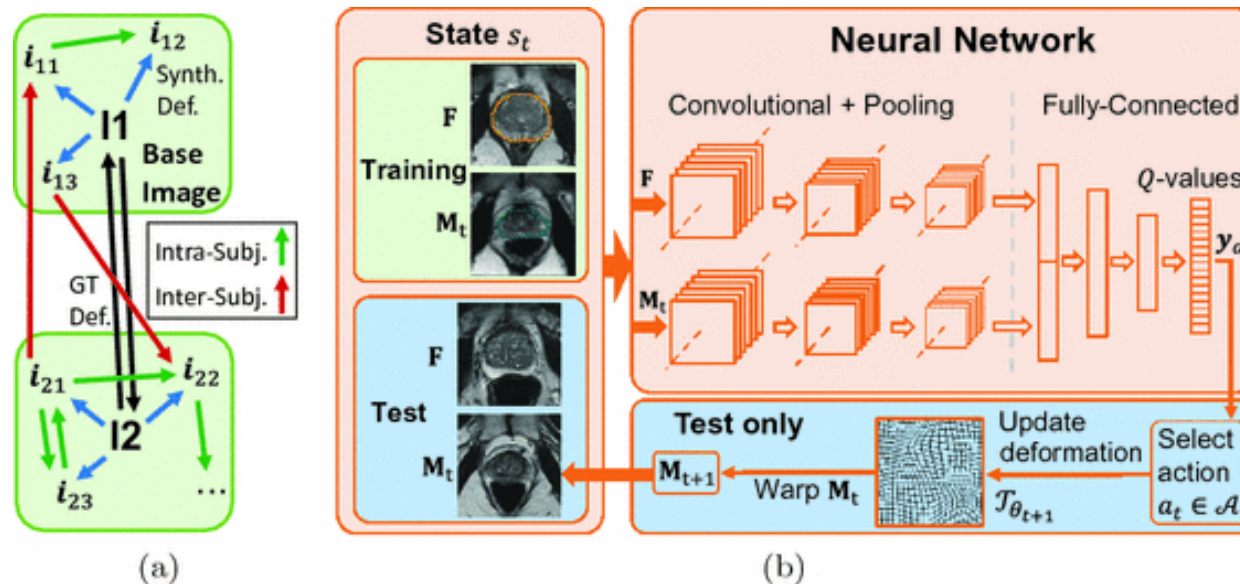
Cumulative sum of prediction errors



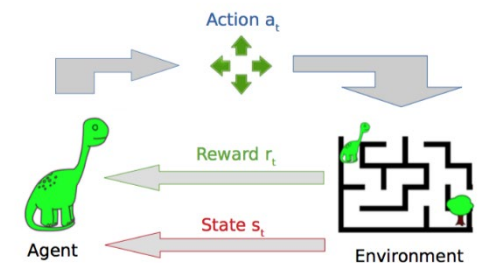
Where are we in the image registration “recipe”?



Example 2: Reinforcement learning for image registration



(a) Training Data Generation: **Synthetic deformations** (blue arrows) and inter-subject GT deformations (black) are used for intra- (green) and inter-subject (red) image pairs for training. (b) Dual-stream network used for Q-value prediction including complete single-stage Markov Decision Process for testing (blue background).



B. Supervised methods

Require many known transformations for training, use ground truth labels to calculate the loss

Fully supervised

2D (FlowNet) vs. 3D approaches (e.g. 3D U-net); mostly patch-based (e.g. 128^3)

- *Generation of ground truth transformations* → many, e.g. Eppenhof et al. (2018)
Pulmonary ct registration through supervised learning with convolutional neural networks (IEEE trans. on med. imaging)
- *Large Deformation Diffeomorphic Metric Mapping (LDDMM)* → Yang et al. (2017)
Quicksilver: Fast Predictive Image Registration - a Deep Learning Approach (NeuroImage)

Weakly supervised

Use overlap between segmentations or a similarity metric between M and F combined with ground truth

- MR-US registration
 - *CNN* → Hu et al. (2018) Weakly-supervised convolutional neural networks for multimodal image registration (Medical Image Analysis)
 - *Generative Adversarial Networks (GANs)* → Yan et al. (2018) Adversarial image registration with application for mr and trus image fusion (arXiv preprint: 1804.11024)

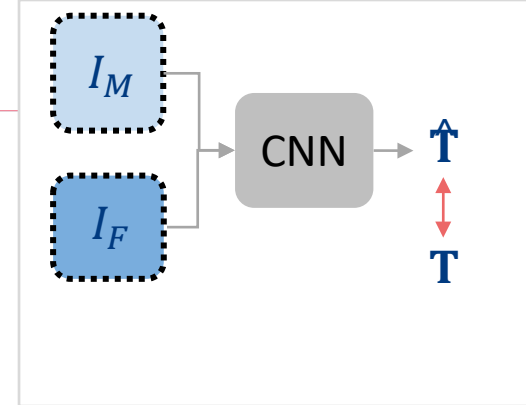
Supervised learning of the transformation requires a ground truth!

Questions:

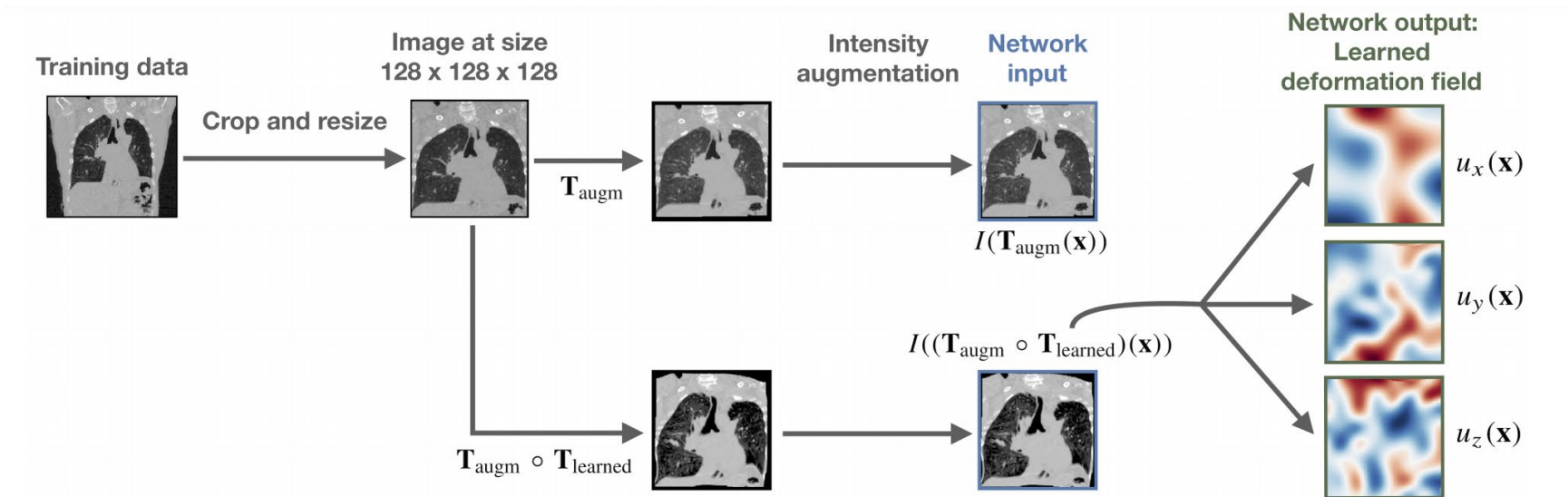
- What is the ground truth of an image registration task?
 - Parametric?
 - Non-parametric?
- How can we acquire this?

B. Supervised transformation estimation

Requires many known transformations for training, use ground truth labels to calculate the loss



Example 1: “On-the-fly” simulation of displacement fields: T_{augm} (Eppenhof & Pluim, 2018)



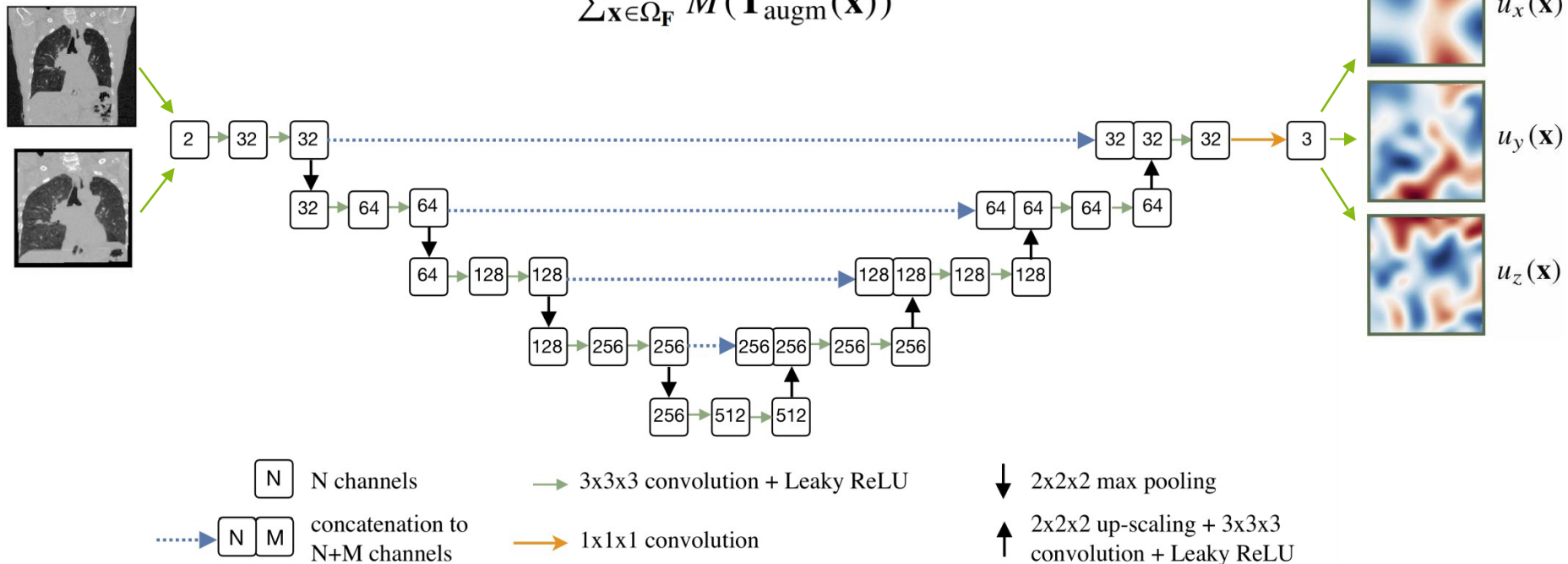
Learning the displacement vector field (Eppenhof & Pluim, 2018)

Binary mask
of the lungs

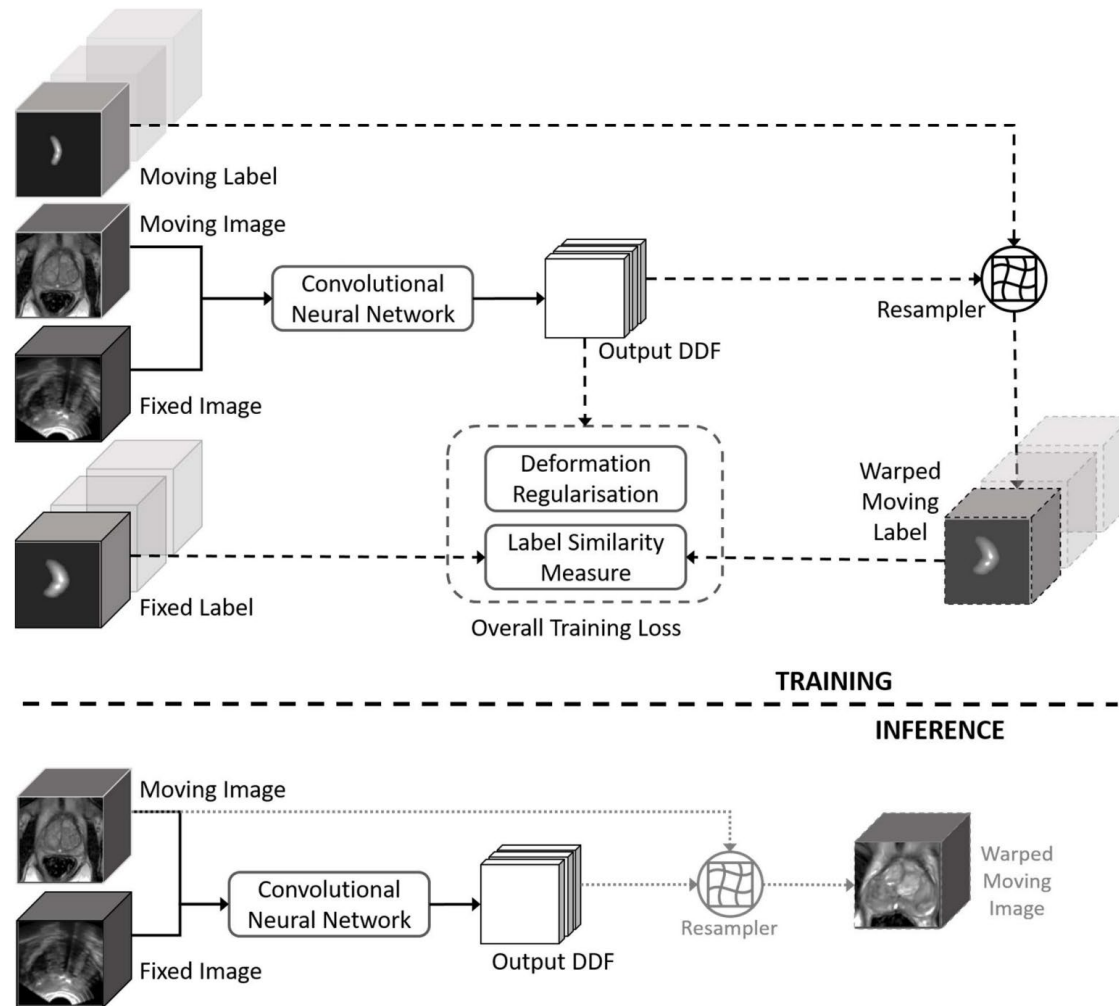
True vector field

Estimated vector field

$$L = \frac{\sum_{\mathbf{x} \in \Omega_F} M(\mathbf{T}_{\text{augm}}(\mathbf{x})) |\mathbf{u}(\mathbf{x}) - \hat{\mathbf{u}}(\mathbf{x})|}{\sum_{\mathbf{x} \in \Omega_F} M(\mathbf{T}_{\text{augm}}(\mathbf{x}))}$$



Example 2: Weakly-supervised CNN for MR-US registration



C. Unsupervised methods

No ground truth needed. Often use a spatial transformer layer.

Variational autoencoders → Krebs et al. (2018) Unsupervised Probabilistic Deformation Modeling for Robust Diffeomorphic Registration. (DLMIA)

Generative Adversarial Networks (GANs) → Tanner et al. (2018) Generative Adversarial Networks for MR-CT Deformable Image Registration (CVPR) & Hu et al. (2018) Adversarial Deformation Regularization for Training Image Registration Neural Networks (MICCAI)

Multi-scale methods:

- **RegNet** → Sokooti et al. (2017) Nonrigid Image Registration Using Multi-scale 3D Convolutional Neural Networks (MICCAI). NB: dual path
- **ConvNet** → De Vos et al. (2018) A deep learning framework for unsupervised affine and deformable image registration (Medical Image Analysis). NB: chain
- **pgCNN** → Eppenhof et al. (2019) Progressive Growing Convolutional Networks for End-to-End Deformable Image Registration (SPIE medical imaging)

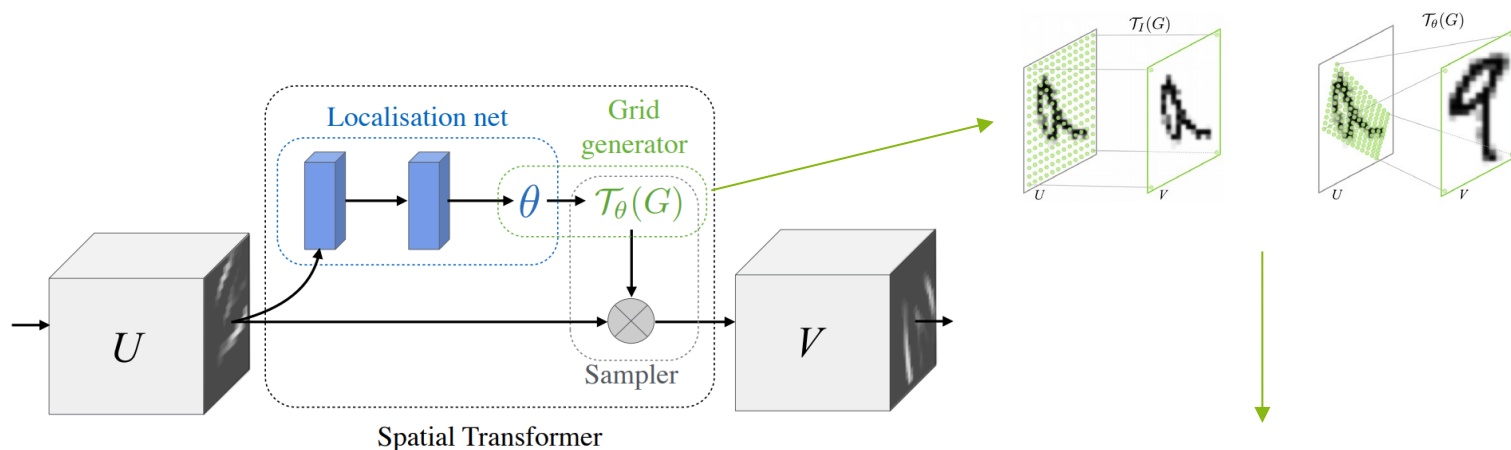
VoxelMorph (U-net) → Balakrishnan et al. (2019) VoxelMorph: A Learning Framework for Deformable Medical Image Registration (IEEE tran.med.imaging)

- **Cycle-consistent VoxelMorph** → Kim et al. (2019) Unsupervised Deformable Image Registration Using Cycle-Consistent CNN (MICCAI)

Spatial transformer networks (Jaderberg et al., NIPS 2015)

Spatial transformer = a learnable module that explicitly allows the spatial manipulation of data within the network

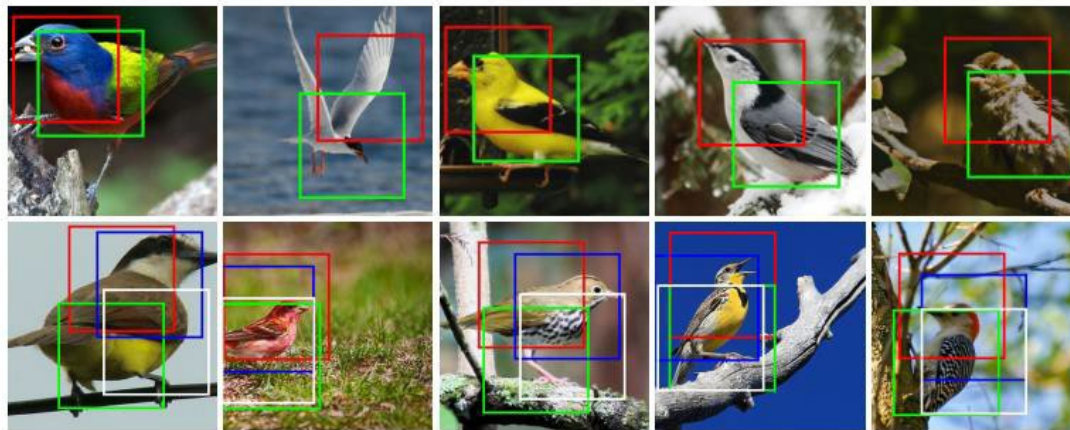
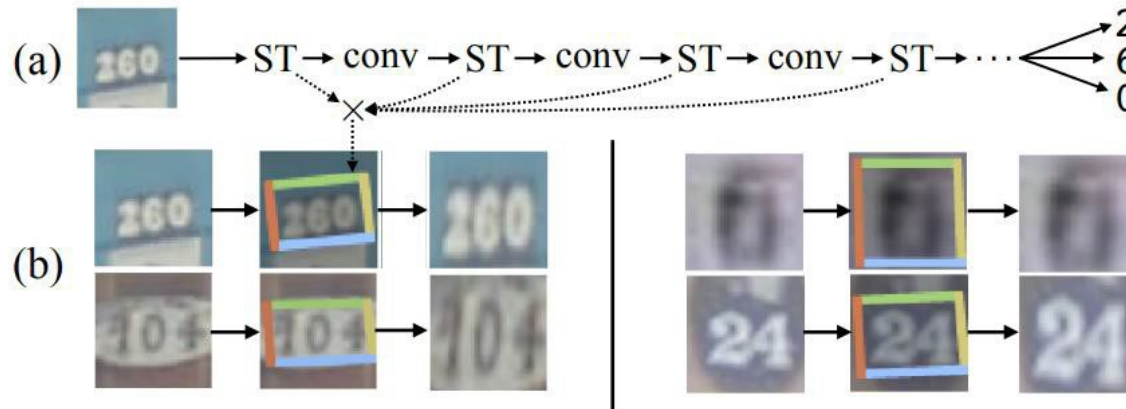
- *Differentiable*
- Can be inserted into existing convolutional neural networks
- Actively transforms feature maps (conditional on the feature map itself)



Example $T_\theta(G)$ for an affine transformation:

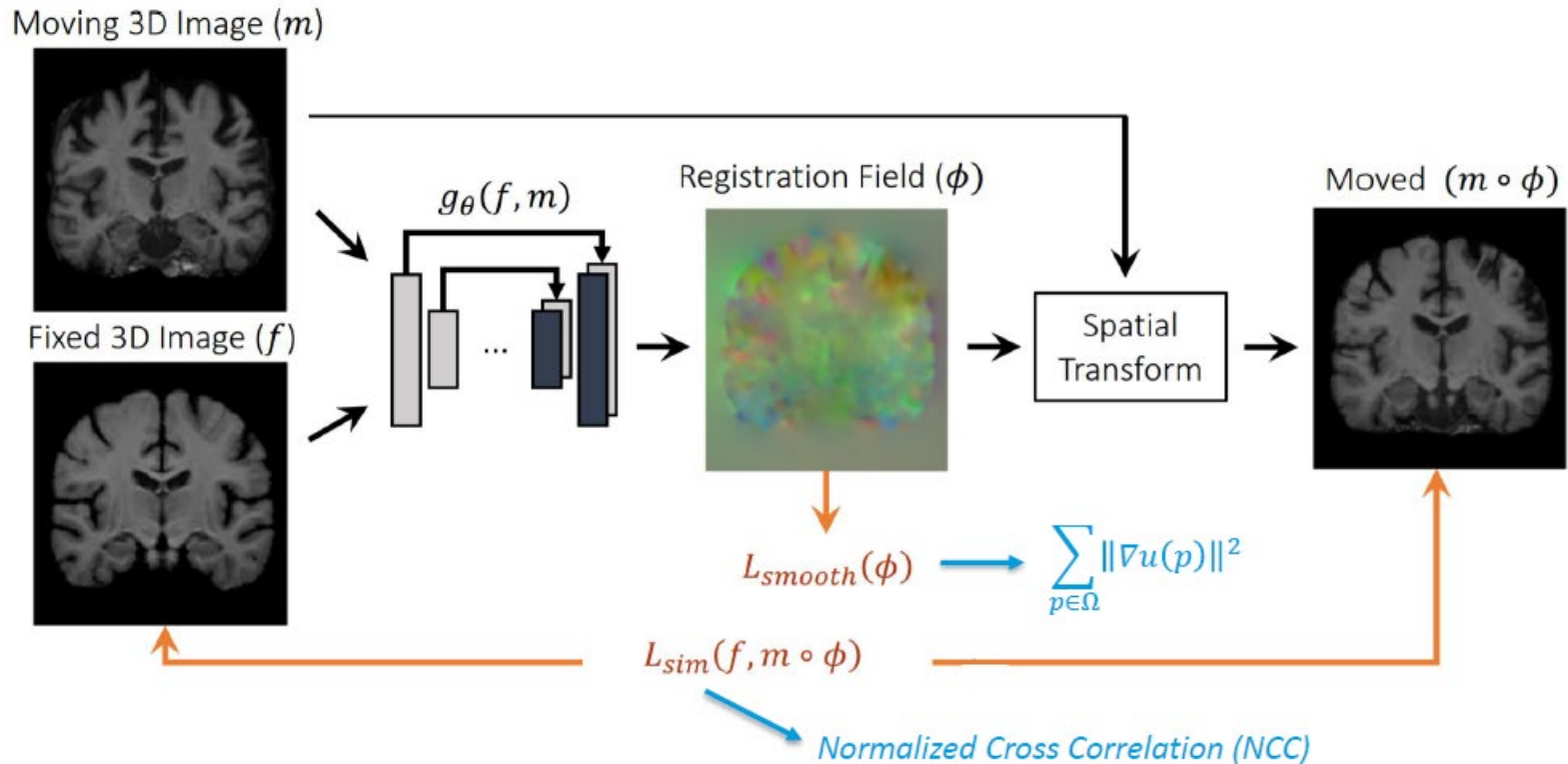
$$\begin{pmatrix} x_i^s \\ y_i^s \end{pmatrix} = T_\theta(G_i) = A_\theta \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix} = \begin{bmatrix} \theta_{11} & \theta_{12} & \theta_{13} \\ \theta_{21} & \theta_{22} & \theta_{23} \end{bmatrix} \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix}$$

CNNs are in essence not invariant to translation, scale, rotation and more generic warping of the input data



VoxelMorph

Example of a popular unsupervised framework for deformable image registration



Summary

- Parametric vs. non-parametric image registration
 - Displacement vector fields
- Formulation of deformable image registration
- Different ways to use deep learning for image registration
 - Deep iterative registration
 - Supervised learning
 - Unsupervised learning
- Disadvantages of deep learning for image registration
(performance, # of training data, ground truth, ...)

