

# Deep learning for medical image registration

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## Outline for today:

- Quick recap of medical image registration
- Introduction non-parametric / deformable image registration
- Deep learning for medical image registration:
  - Deep iterative registration
  - Supervised methods
  - Unsupervised (optimization-based) methods

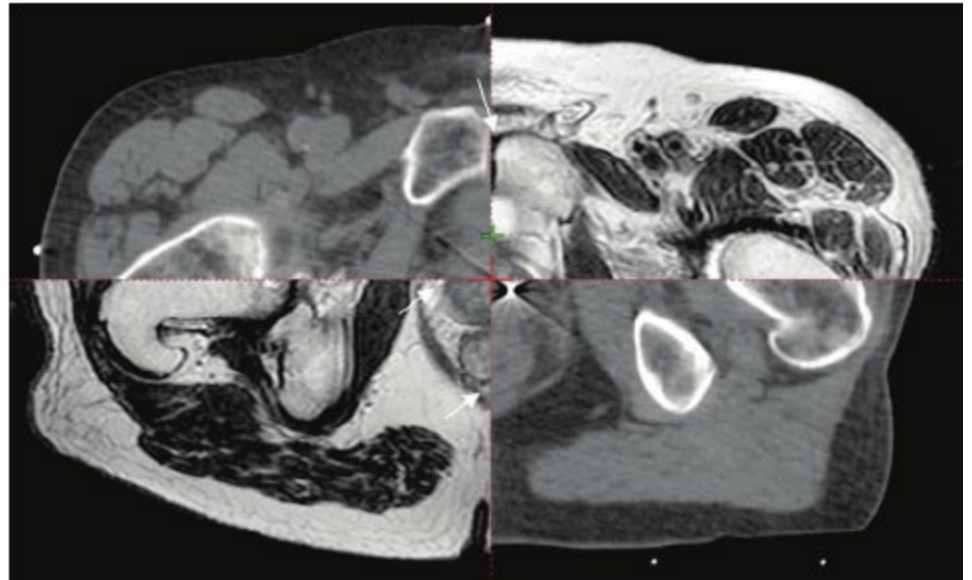
## Recap: medical image registration

Why important?

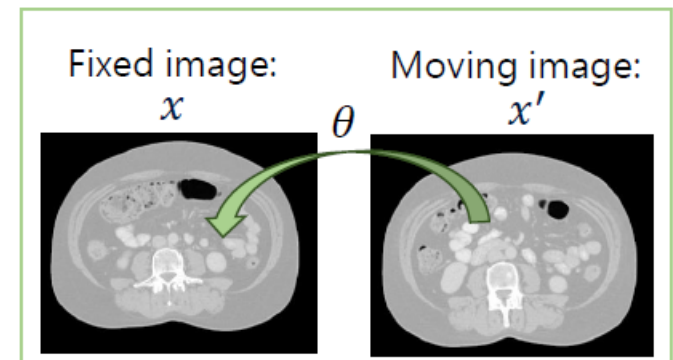
- Multi-modal registration (e.g. CT on MRI)
- Inter-subject (e.g. atlas registration)
- Longitudinal (e.g. treatment evaluation)

*Remaining challenges:*

- Large 3D volumes
- Accuracy vs. efficiency
- Intensity inhomogeneities and discontinuities
- Outlier rejection



## Medical image registration: general “recipe”



**Transformation model:**  
(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

**Similarity measure:**  
(e.g. SSD, CC, MI, MSE)

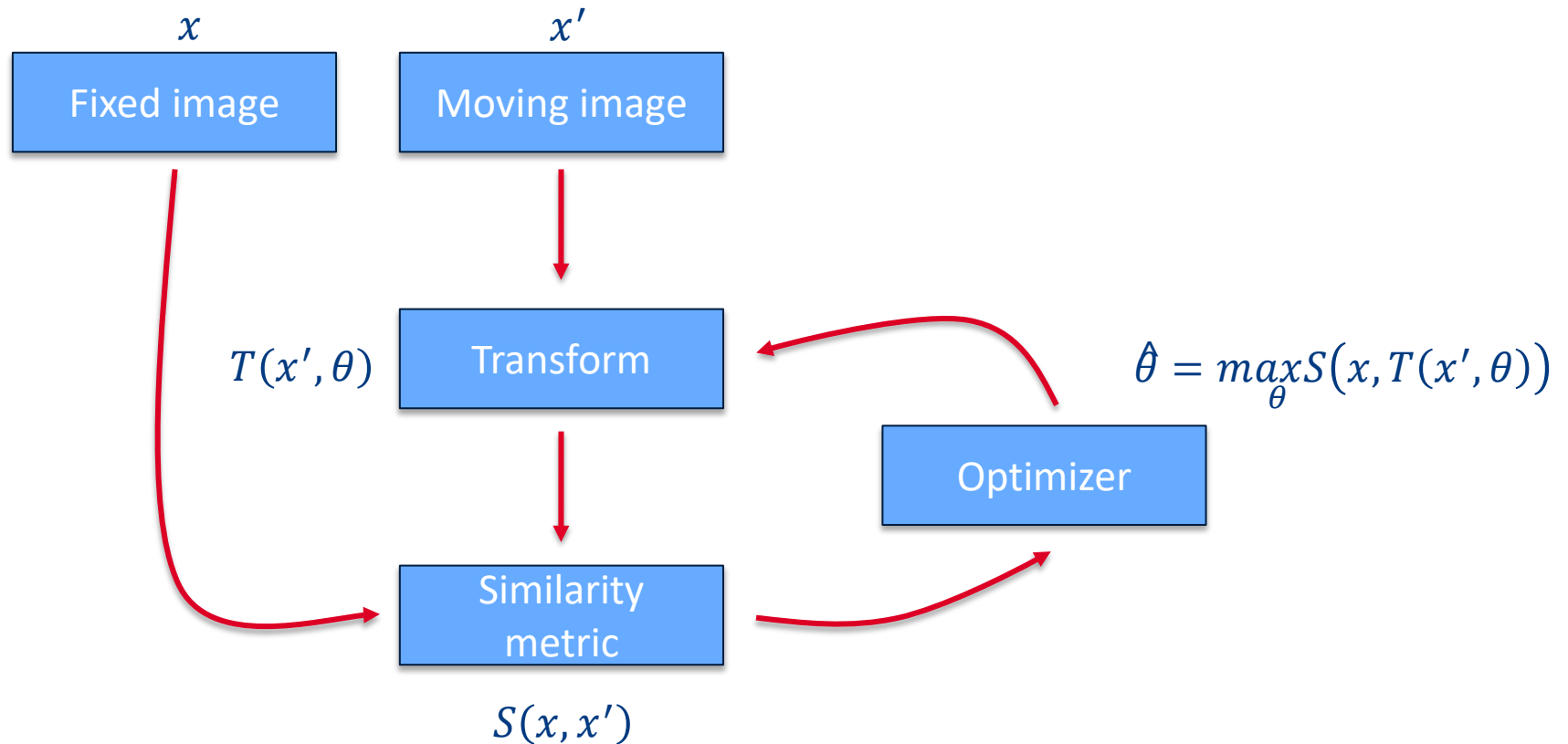
$$S(x, x')$$

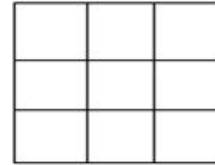
**Image  
registration**

**Optimization:**

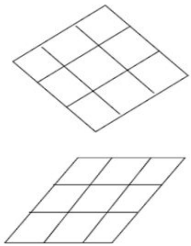
$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

## Finding the optimal transformation



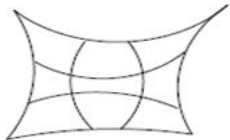


## Transformation models



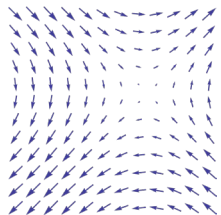
### Rigid & Affine

- Point or feature-based (e.g. landmarks, fiducials)
- Intensity-based
- Gradient/edge-based



### Non-linear

- Linear or higher order polynomials
- Spline-based



### Non-parametric / deformable

- Allowing each image element to be displaced arbitrarily

## Rigid transformations

- Translation
- Rotation

$$\mathbf{x}' = \mathbf{R}\mathbf{x} + \mathbf{t}$$

$$\mathbf{t} = \begin{bmatrix} t_x \\ t_y \end{bmatrix}$$

$$\mathbf{R} = \begin{bmatrix} \cos(\phi) & -\sin(\phi) \\ \sin(\phi) & \cos(\phi) \end{bmatrix}$$

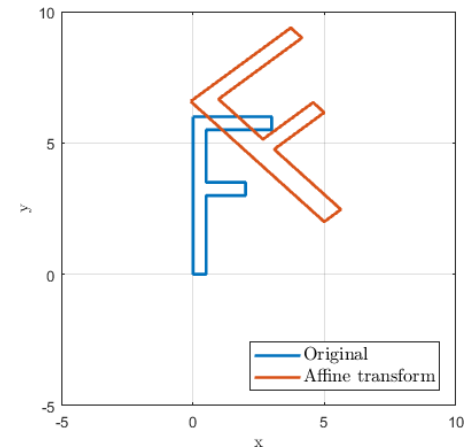
## Affine transformations: translation, rotations and

- Scaling
- Shearing

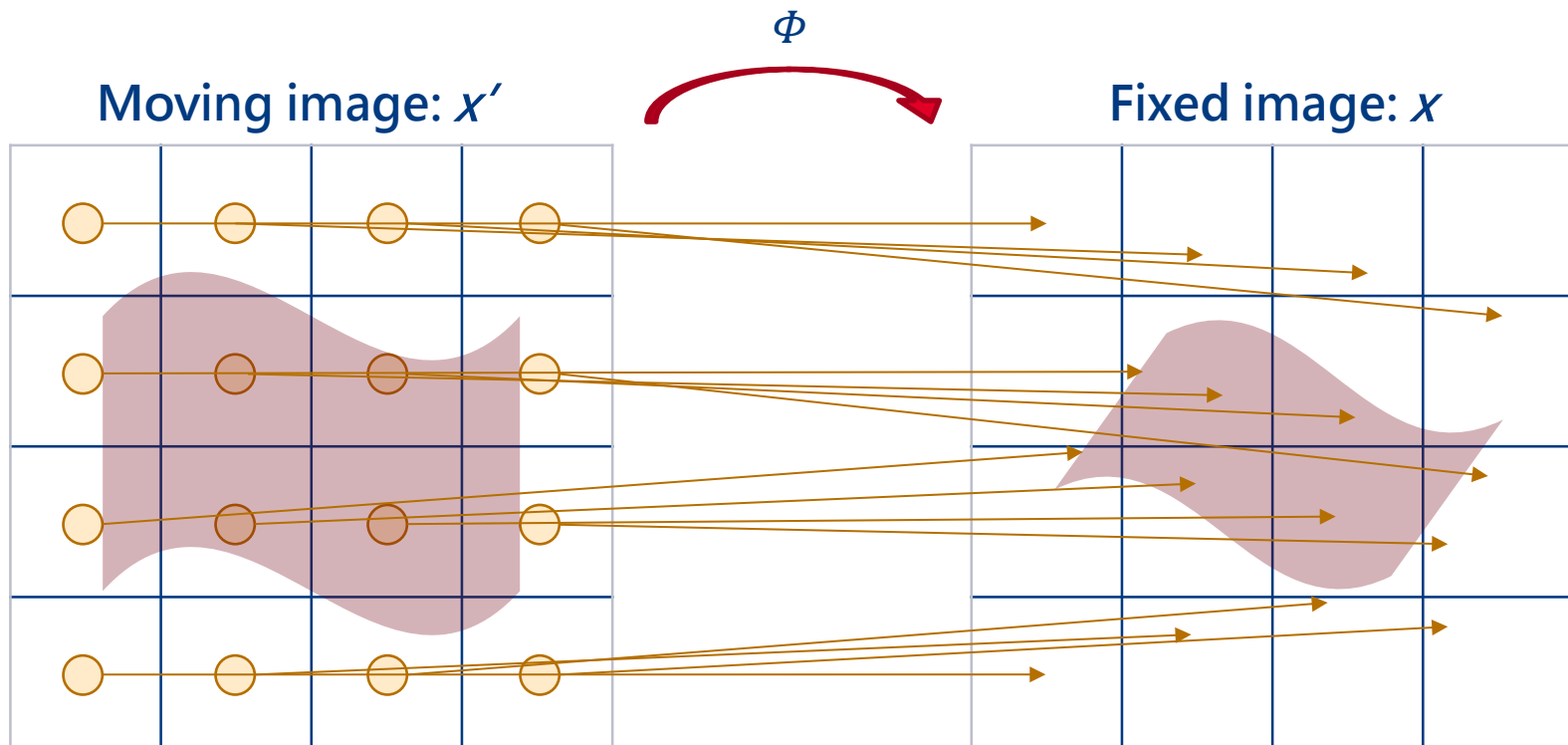
$$\mathbf{x}' = \mathbf{A}\mathbf{x} + \mathbf{t}$$

$$\mathbf{S} = \begin{bmatrix} s_x & 0 \\ 0 & s_y \end{bmatrix}$$

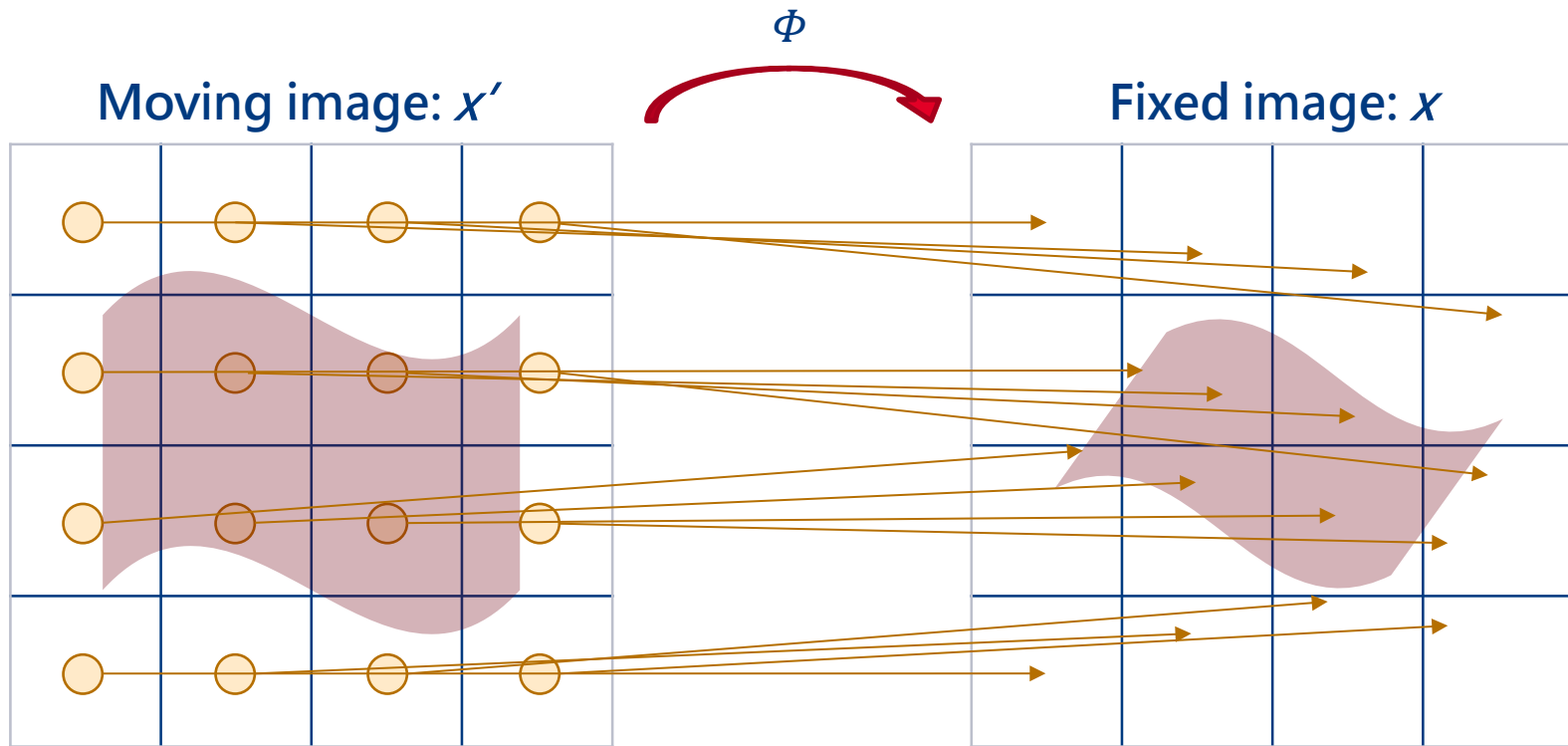
$$\mathbf{H} = \begin{bmatrix} 1 & h_x \\ h_y & 1 \end{bmatrix}$$



**Displacement (vector) field (DVF)** = Dense set of vectors representing the displacement in a given spatial domain





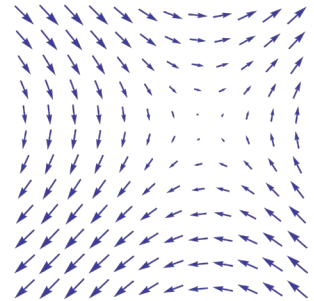


Deformation:  $\varphi = Id + u, \varphi: \Omega \rightarrow \mathbb{R}^d$   
 or point-wise:  $\varphi(x) = x + u(x)$

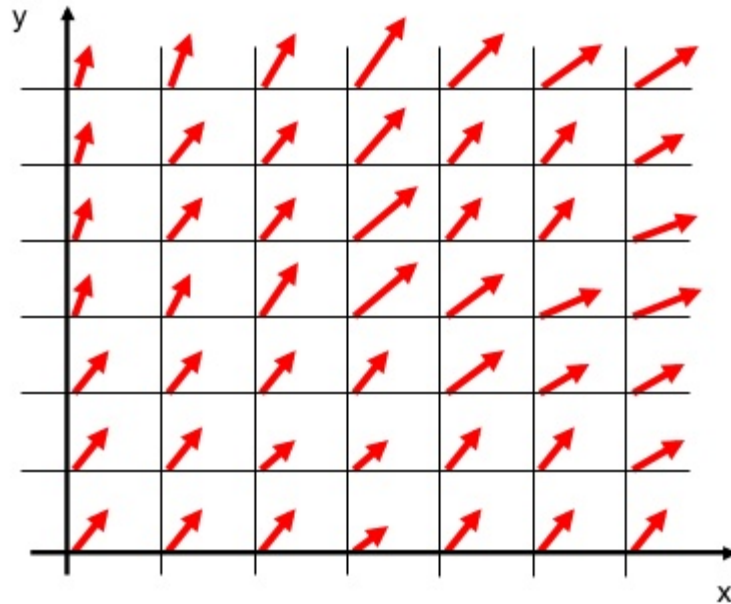
Displacement:

$$u: \Omega \rightarrow \mathbb{R}^d$$

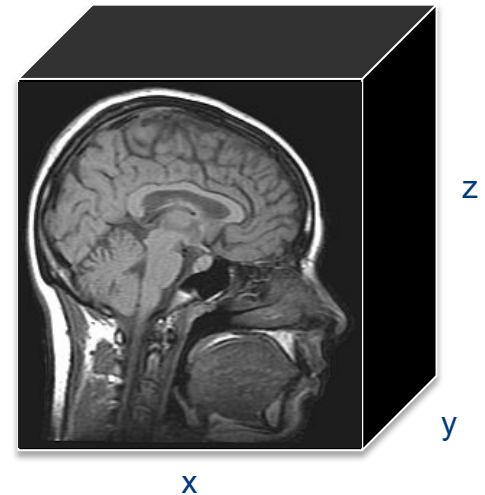
e.g.  $u$   
 $= [u_x, u_y, u_z]$



## Deformable image registration: how many free parameters (DOF) in 3D?



Typical spatial resolution of a  
3D medical image  
(MRI: e.g.  $1.5 \times 1.5 \times 4 \text{ mm}^3$  voxels)



$$\text{DOF} = 3 \cdot N_x \cdot N_y \cdot N_z (!)$$

Deformable image registration is still a very active area of research, and many different deformable registration models exist:

- Free-form deformation model
- Optical flow
- Demons
- Fluid flow
- Diffeomorphisms
- ...

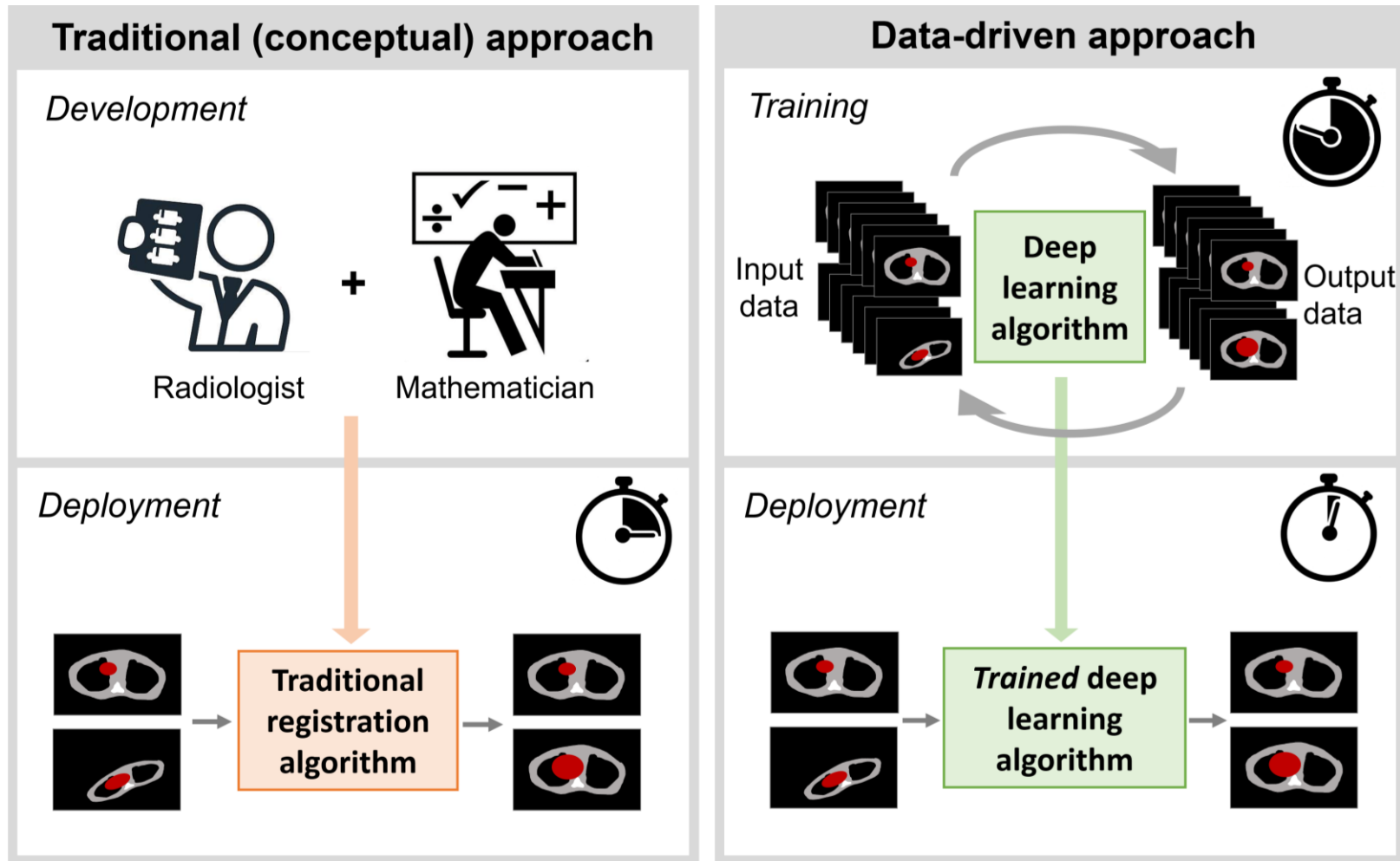
Note that the details of these models and their implementations are beyond the scope of this course.

## Learning goals of this lecture

The students should be able to:

- Explain the difference between parametric and non-parametric image registration models
- Formulate deformable image registration as an optimization problem
- Understand displacement vector fields
- Explain the difference between supervised and unsupervised learning
- Understand why deep learning is an interesting technique to solve medical image registration tasks
- Understand the different ways in which deep learning can be used to perform (deformable) image registration

## Why focus on deep learning for medical image registration?



## Machine learning – different training strategies

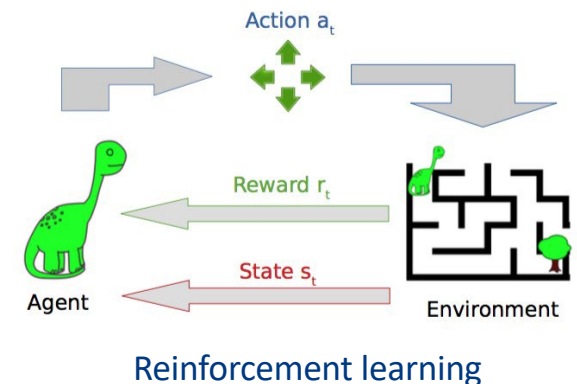
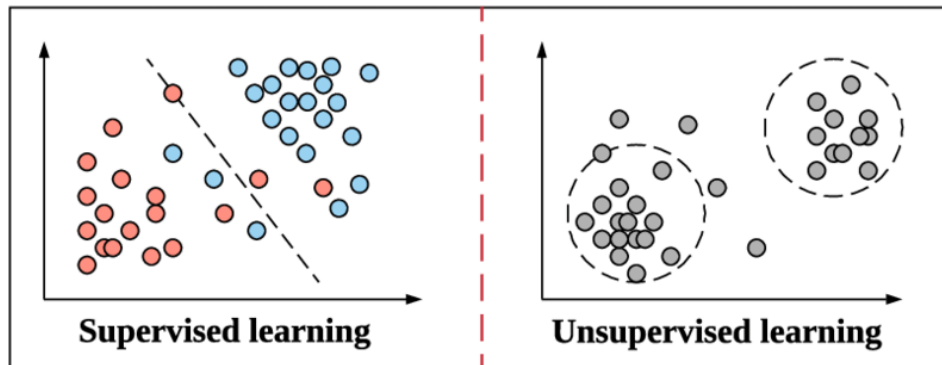
**Supervised learning** = develop predictive model based on input and output data (i.e., ground truth, “labels”)

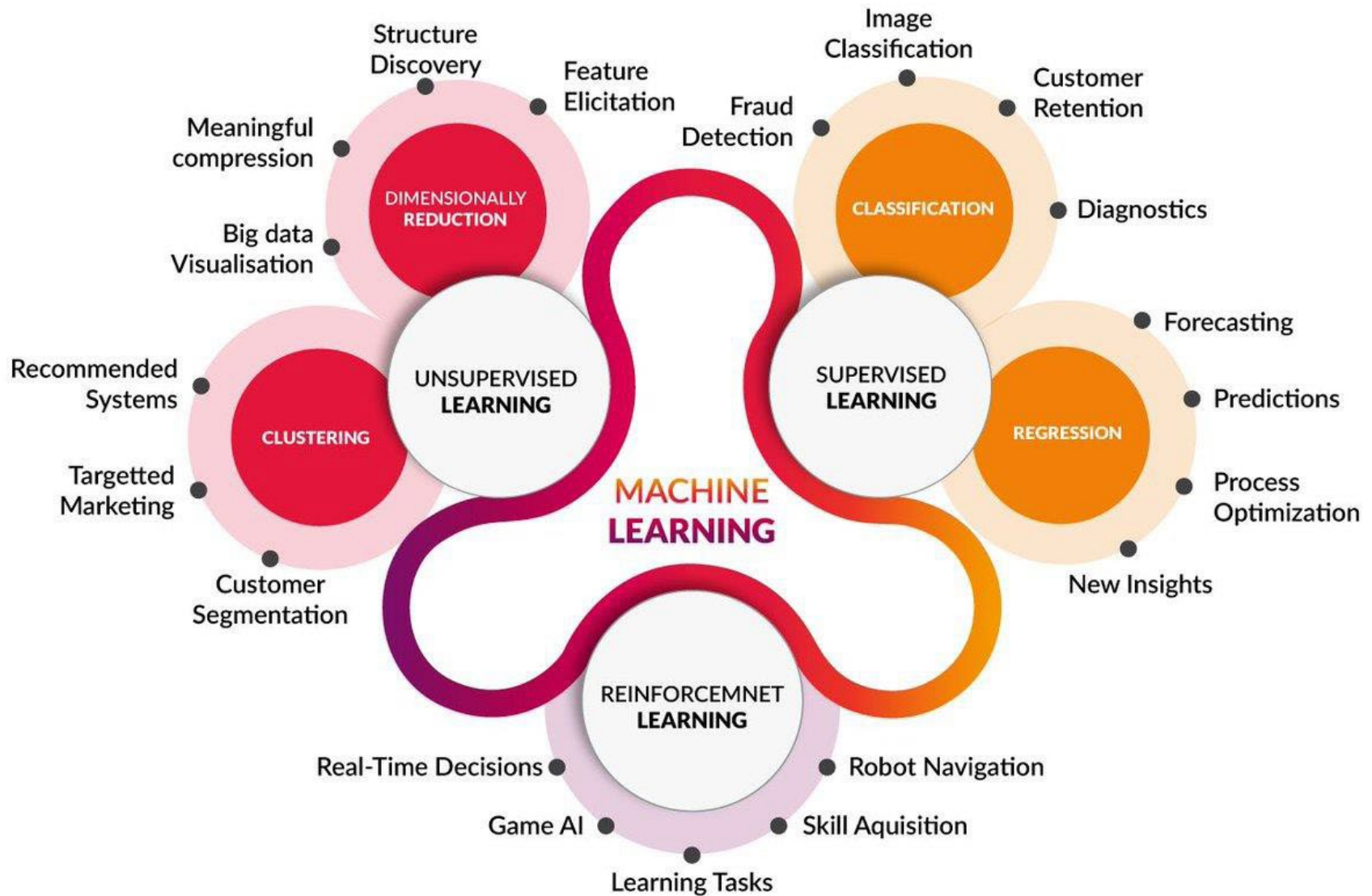
Examples: classification (e.g., skin lesion classification), regression (segmentation of vessel structures)

**Unsupervised learning** = group or interpret data based on input data alone

Example: clustering (e.g., k-means)

*NB: also semi-supervised learning and reinforcement learning, not part of this course.*





## Learning image registration: how does it work?

Problem: how can we obtain the ground truth displacement ?

### A. Deep iterative registration

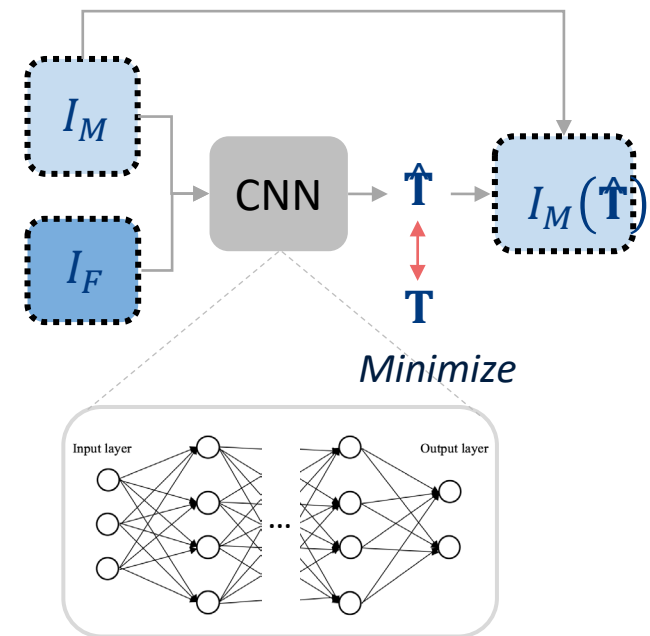
- Learn a component of a classical registration method

### B. Supervised transformation estimation

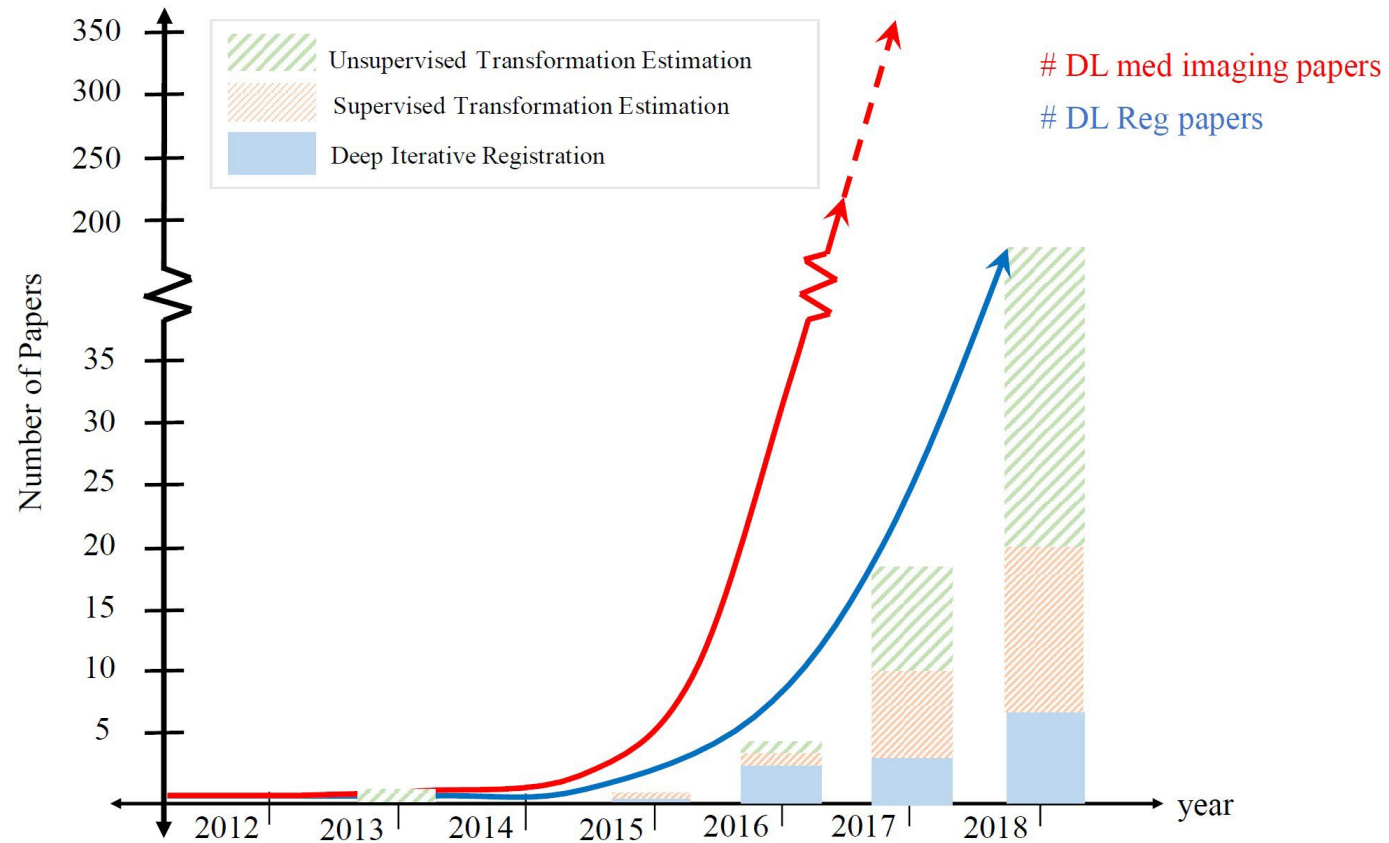
- Obtain using classical registration method
- or make synthetic ground truth

### C. Unsupervised transformation estimation

- Use similarity metric to judge







## A. Deep iterative registration

Use a traditional registration method and learn one component

### Automatically extract (learn) similarity features

- *Unimodal*: Wu et al. (2013) Unsupervised deep feature learning for deformable registration of mr brain images (MICCAI); Wu et al. (2016) Scalable high-performance image registration framework by unsupervised deep feature representations learning (IEEE Transactions on Biomedical Engineering); Eppenhof et al. (2018) Error estimation of deformable image registration of pulmonary ct scans using convolutional neural networks (Journal of Medical Imaging)
- *Multimodal*: Mostly *rigid registration*; learn a similarity metric to evaluate or register multimodal images using gradient descent. E.g. Cheng et al. (2016&2018) Deep similarity learning for multimodal medical images (MICCAI)

### Reinforcement learning

Mostly used for *rigid registration*

- Low-resolution transformation model for deformable registration  
Krebs et al. (2017) Robust non-rigid registration through agent-based action learning (MICCAI)

## Where are we in the image registration “recipe”?

Transformation model:  
(e.g., rigid, affine, deformable)

$$T(x', \theta)$$

Similarity measure:  
(e.g. SSD, CC, MI, MSE)

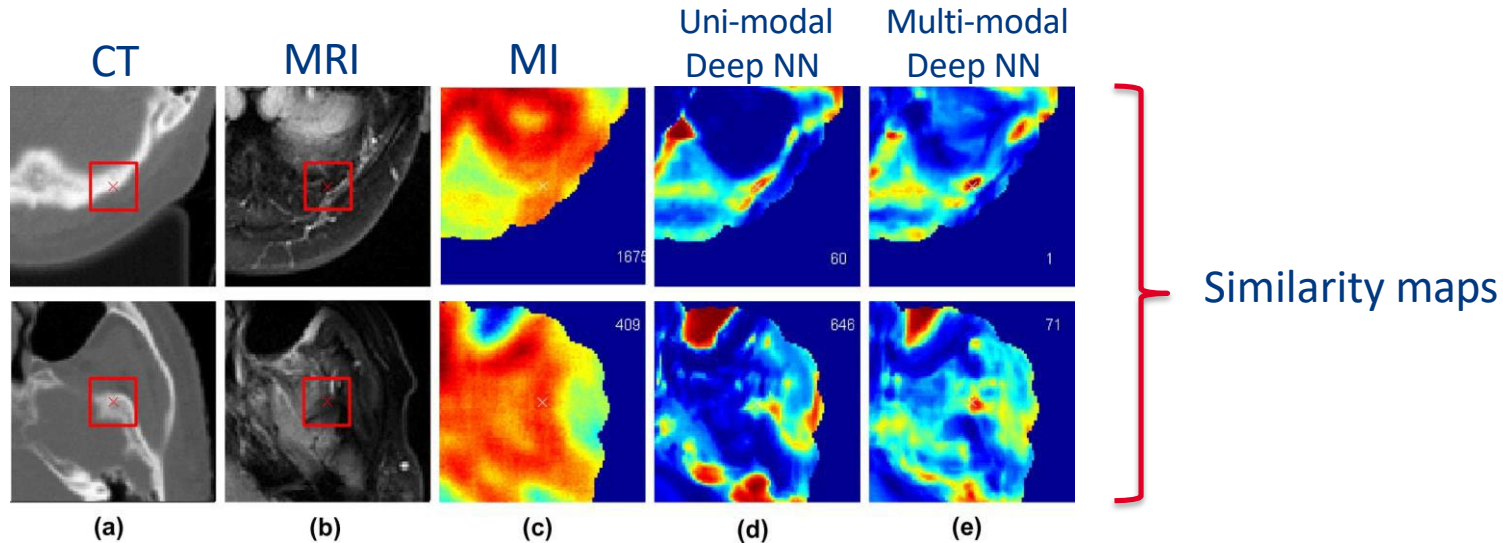
$$S(x, x')$$

Image  
registration

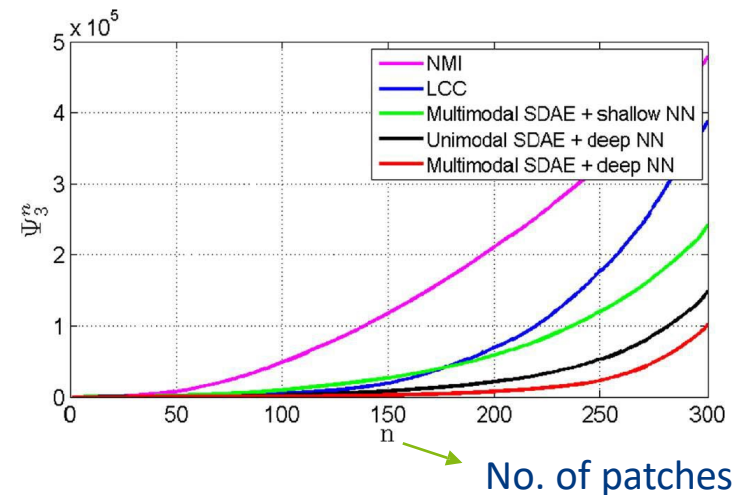
Optimization:

$$\hat{\theta} = \max_{\theta} S(x, T(x', \theta))$$

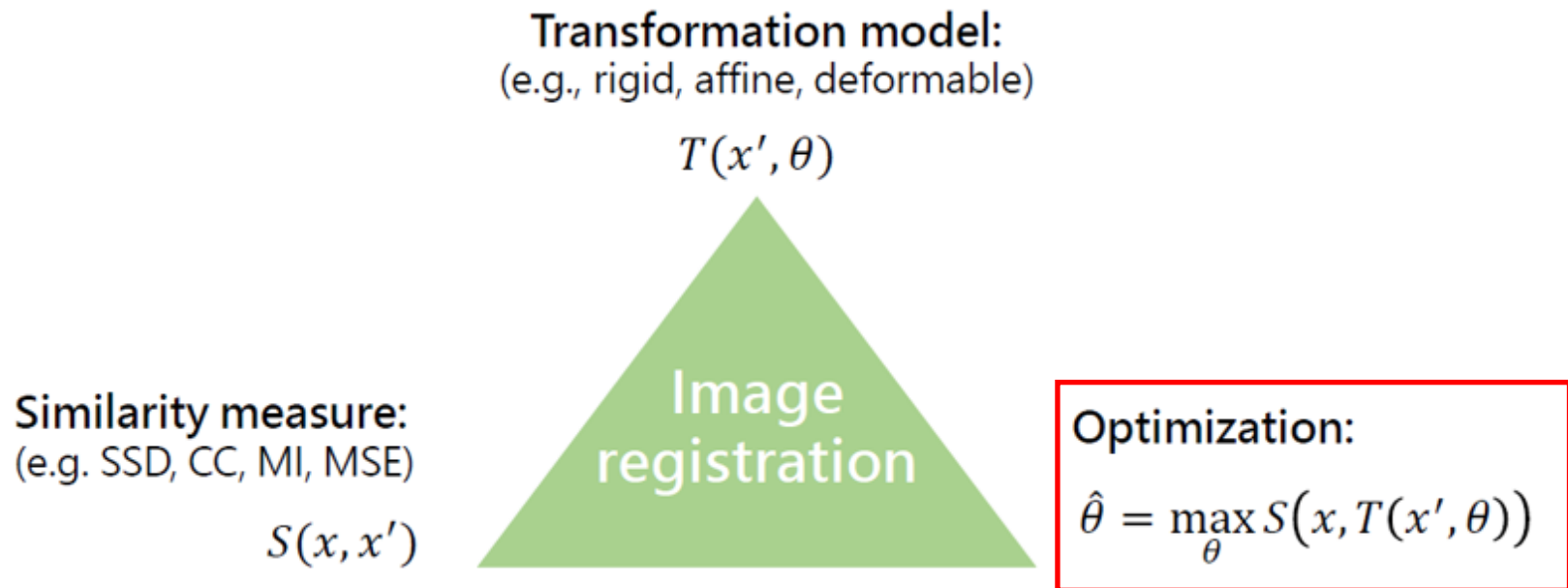
## Example 1: Learning multimodal feature extraction (Haskins et al., 2019)



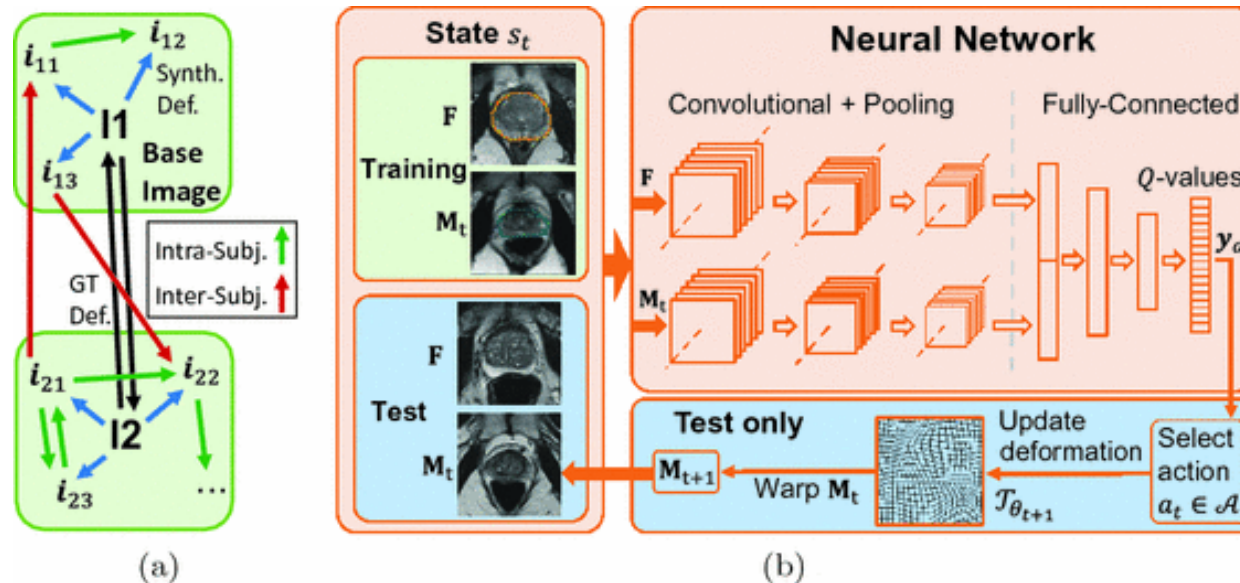
Cumulative sum of prediction errors



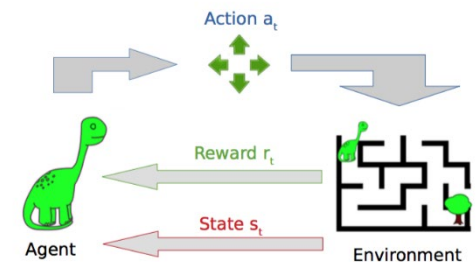
## Where are we in the image registration “recipe”?



## Example 2: Reinforcement learning for image registration



(a) Training Data Generation: **Synthetic deformations** (blue arrows) and inter-subject GT deformations (black) are used for intra- (green) and inter-subject (red) image pairs for training. (b) Dual-stream network used for Q-value prediction including complete single-stage Markov Decision Process for testing (blue background).



## B. Supervised methods

Require many known transformations for training, use ground truth labels to calculate the loss

### Fully supervised

2D (FlowNet) vs. 3D approaches (e.g. 3D U-net); mostly patch-based (e.g.  $128^3$ )

- *Generation of ground truth transformations* → many, e.g. Eppenhof et al. (2018)  
Pulmonary ct registration through supervised learning with convolutional neural networks (IEEE trans. on med. imaging)
- *Large Deformation Diffeomorphic Metric Mapping (LDDMM)* → Yang et al. (2017)  
Quicksilver: Fast Predictive Image Registration - a Deep Learning Approach (NeuroImage)

### Weakly supervised

Use overlap between segmentations or a similarity metric between  $M$  and  $F$  combined with ground truth

- MR-US registration
  - *CNN* → Hu et al. (2018) Weakly-supervised convolutional neural networks for multimodal image registration (Medical Image Analysis)
  - *Generative Adversarial Networks (GANs)* → Yan et al. (2018) Adversarial image registration with application for mr and trus image fusion (arXiv preprint: 1804.11024)

Supervised learning of the transformation requires a ground truth!

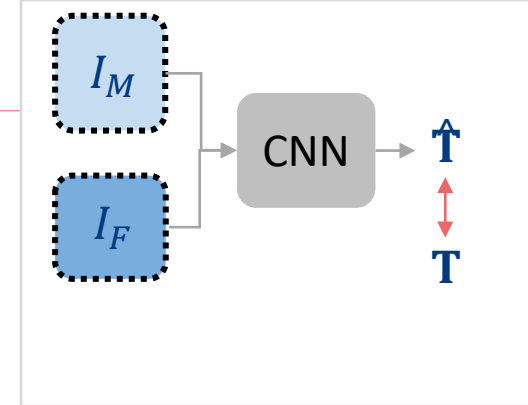
Questions:

- What is the ground truth of an image registration task?
  - Parametric?
  - Non-parametric?
- How can we acquire this?

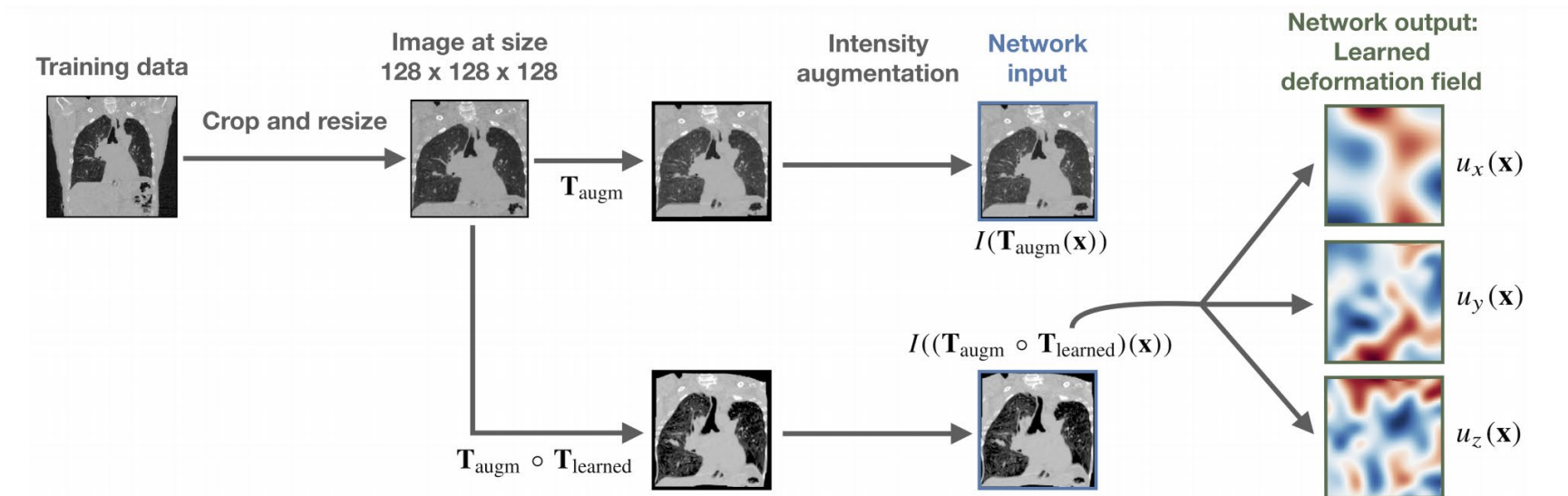


## B. Supervised transformation estimation

Requires many known transformations for training, use ground truth labels to calculate the loss



Example 1: “On-the-fly” simulation of displacement fields:  $T_{augm}$  (Eppenhof & Pluim, 2018)



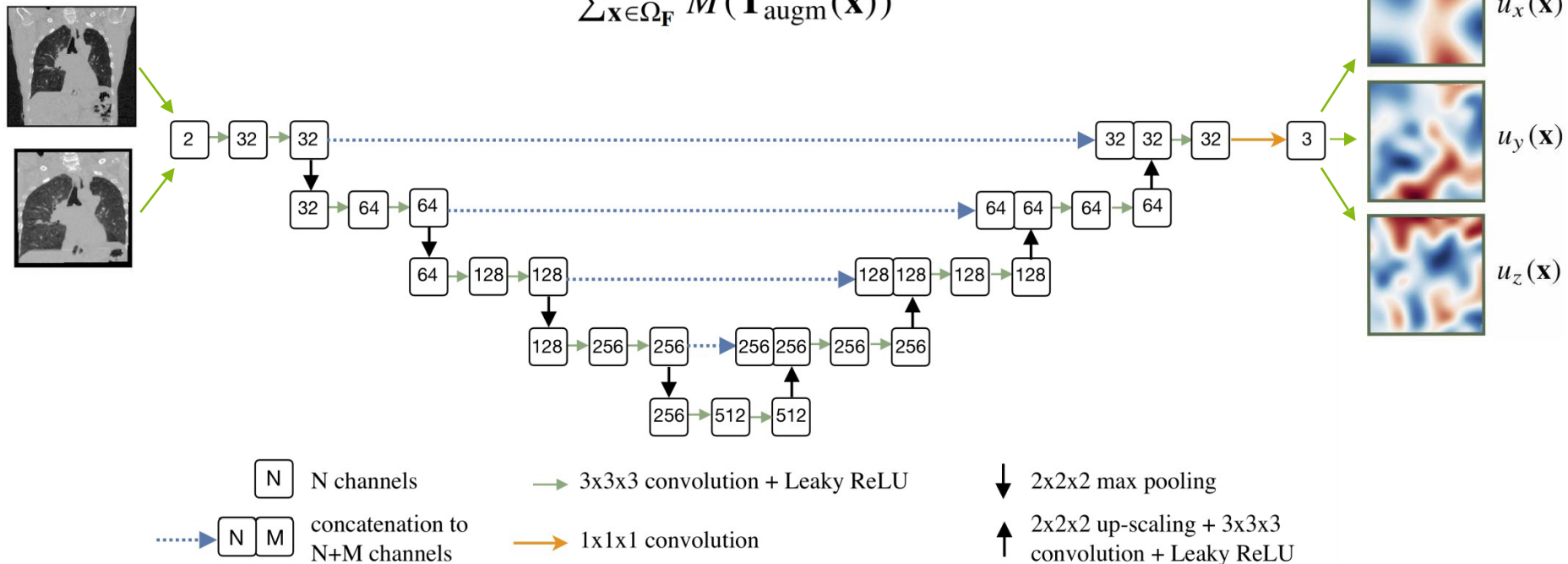
## Learning the displacement vector field (Eppenhof & Pluim, 2018)

Binary mask  
of the lungs

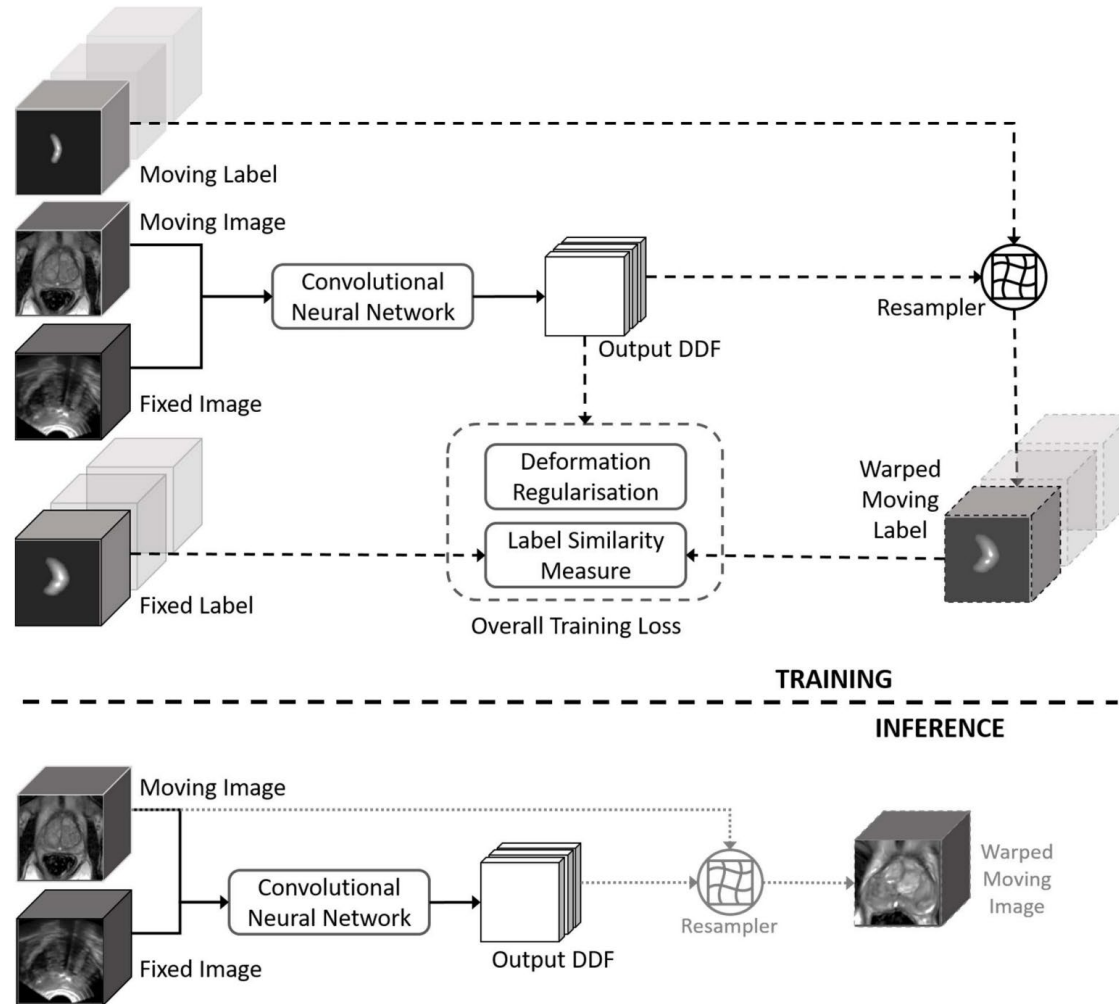
True vector field

Estimated vector field

$$L = \frac{\sum_{\mathbf{x} \in \Omega_F} M(\mathbf{T}_{\text{augm}}(\mathbf{x})) |\mathbf{u}(\mathbf{x}) - \hat{\mathbf{u}}(\mathbf{x})|}{\sum_{\mathbf{x} \in \Omega_F} M(\mathbf{T}_{\text{augm}}(\mathbf{x}))}$$



## Example 2: Weakly-supervised CNN for MR-US registration



## C. Unsupervised methods

No ground truth needed. Often use a spatial transformer layer.

**Variational autoencoders** → Krebs et al. (2018) Unsupervised Probabilistic Deformation Modeling for Robust Diffeomorphic Registration. (DLMIA)

**Generative Adversarial Networks (GANs)** → Tanner et al. (2018) Generative Adversarial Networks for MR-CT Deformable Image Registration (CVPR) & Hu et al. (2018) Adversarial Deformation Regularization for Training Image Registration Neural Networks (MICCAI)

### Multi-scale methods:

- **RegNet** → Sokooti et al. (2017) Nonrigid Image Registration Using Multi-scale 3D Convolutional Neural Networks (MICCAI). NB: dual path
- **ConvNet** → De Vos et al. (2018) A deep learning framework for unsupervised affine and deformable image registration (Medical Image Analysis). NB: chain
- **pgCNN** → Eppenhof et al. (2019) Progressive Growing Convolutional Networks for End-to-End Deformable Image Registration (SPIE medical imaging)

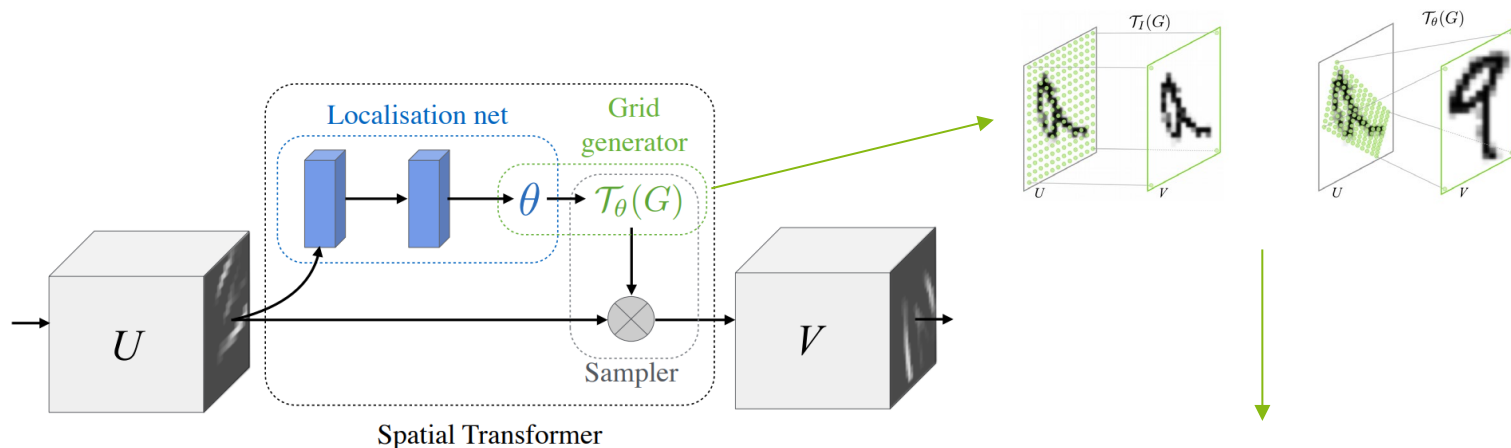
**VoxelMorph (U-net)** → Balakrishnan et al. (2019) VoxelMorph: A Learning Framework for Deformable Medical Image Registration (IEEE tran.med.imaging)

- **Cycle-consistent VoxelMorph** → Kim et al. (2019) Unsupervised Deformable Image Registration Using Cycle-Consistent CNN (MICCAI)

## Spatial transformer networks (Jaderberg et al., NIPS 2015)

**Spatial transformer** = a learnable module that explicitly allows the spatial manipulation of data within the network

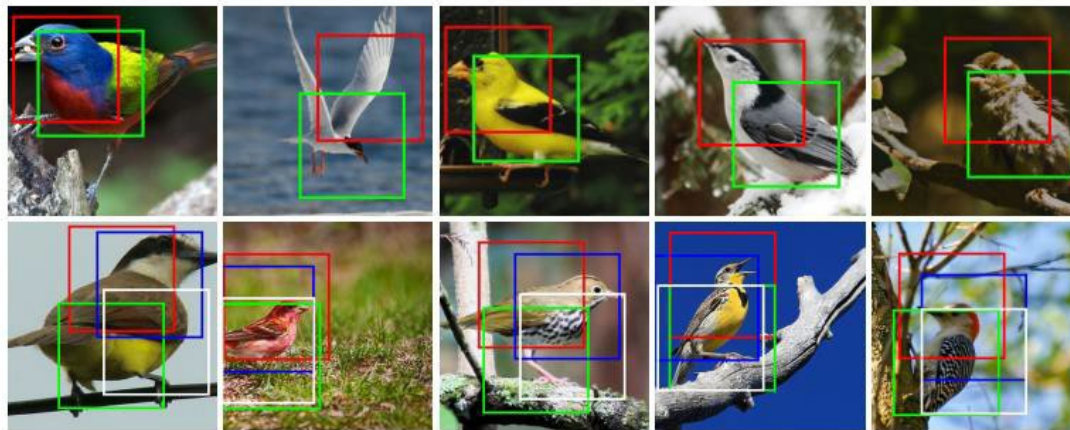
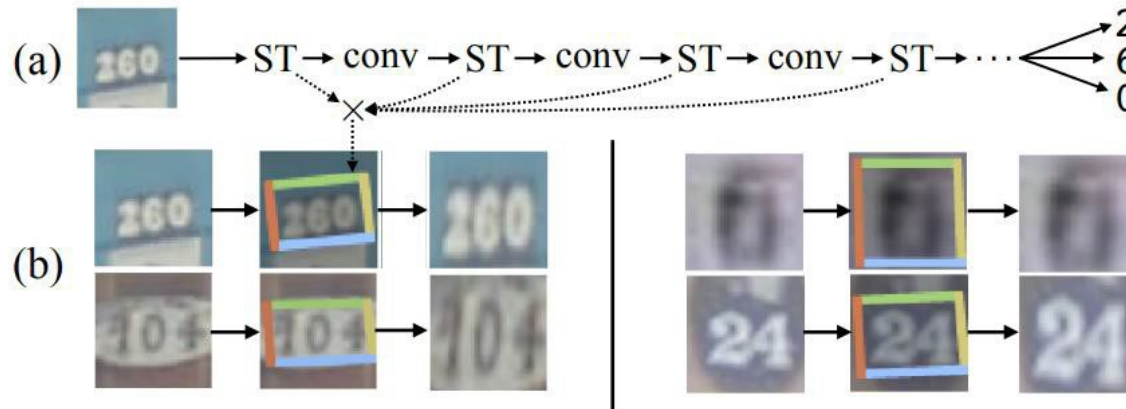
- *Differentiable*
- Can be inserted into existing convolutional neural networks
- Actively transforms feature maps (conditional on the feature map itself)



Example  $T_\theta(G)$  for an affine transformation:

$$\begin{pmatrix} x_i^s \\ y_i^s \end{pmatrix} = T_\theta(G_i) = A_\theta \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix} = \begin{bmatrix} \theta_{11} & \theta_{12} & \theta_{13} \\ \theta_{21} & \theta_{22} & \theta_{23} \end{bmatrix} \begin{pmatrix} x_i^t \\ y_i^t \\ 1 \end{pmatrix}$$

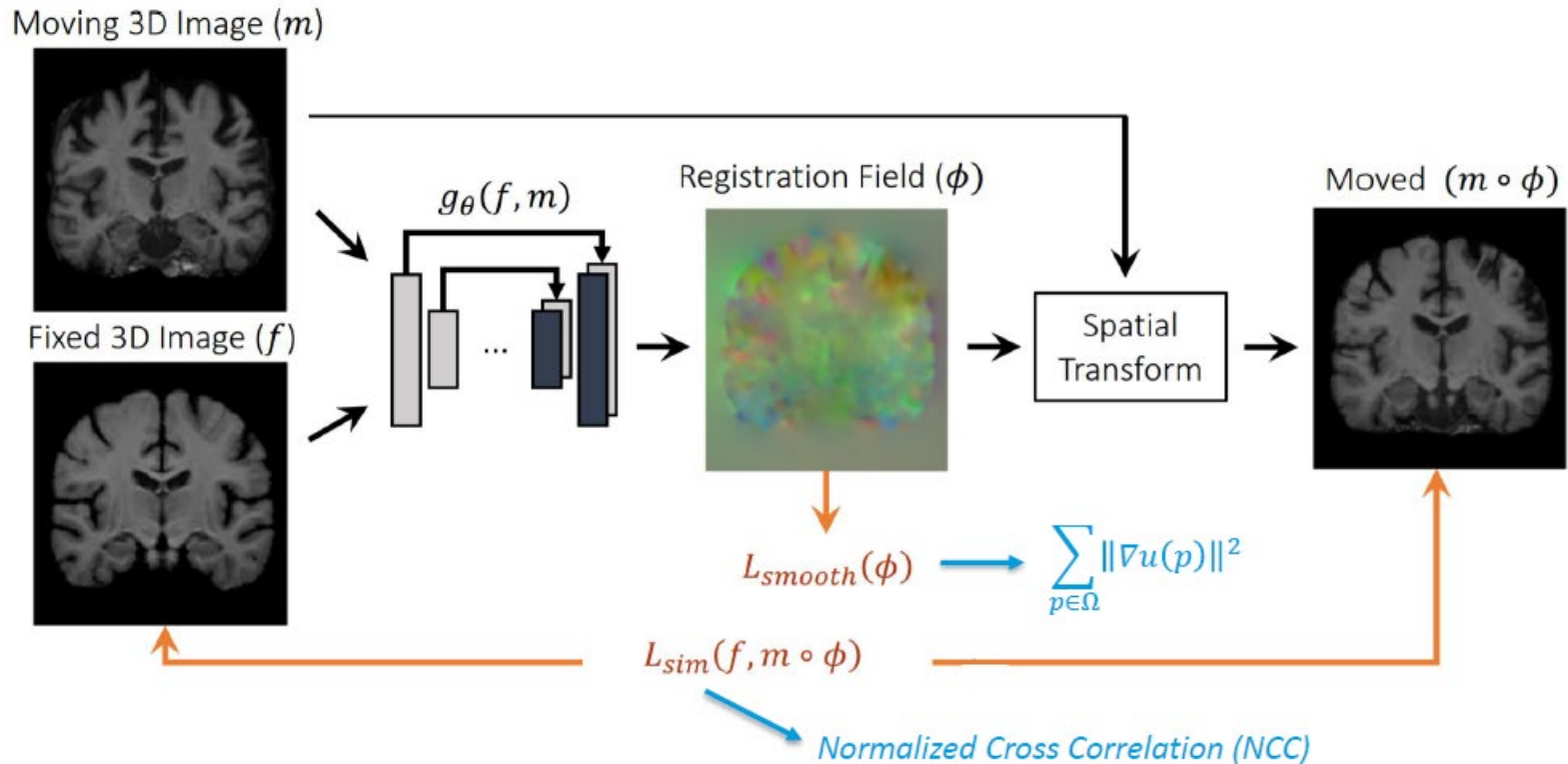
CNNs are in essence not invariant to translation, scale, rotation and more generic warping of the input data





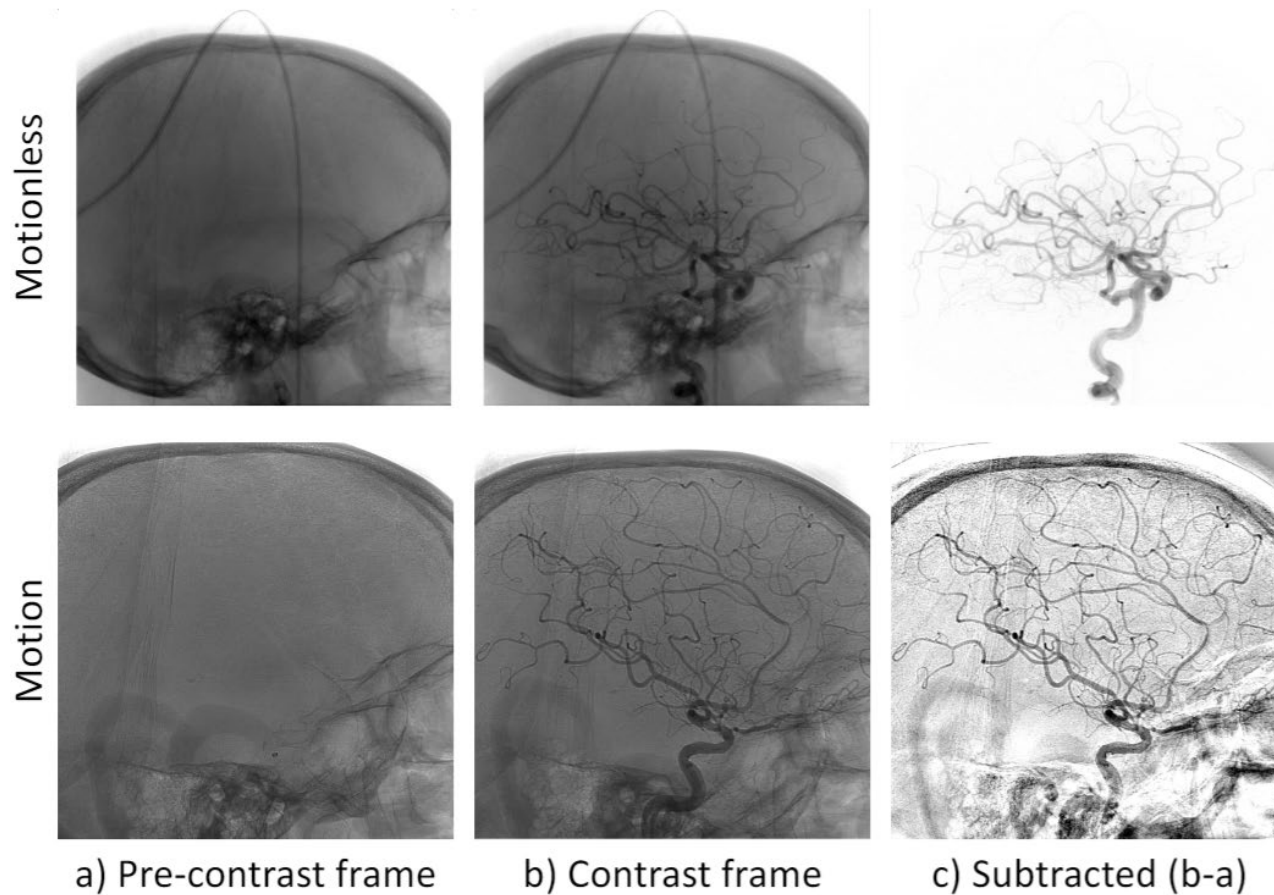
## VoxelMorph

Example of a popular unsupervised framework for deformable image registration

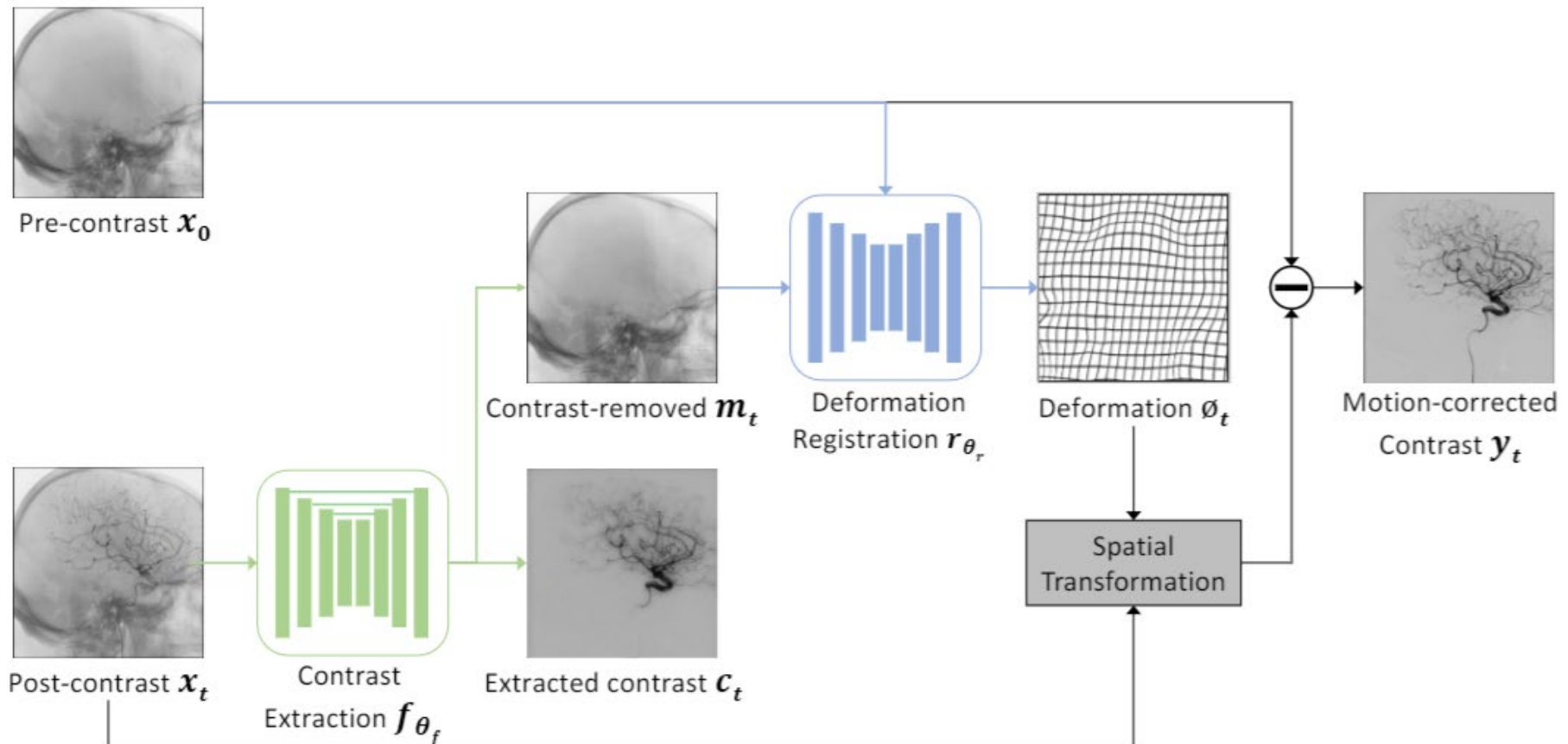


## Example from my own research:

Deformable registration of motion correction in brain digital subtraction angiography







## Summary

- Parametric vs. non-parametric image registration
  - Displacement vector fields
- Formulation of deformable image registration
- Different ways to use deep learning for image registration
  - Deep iterative registration
  - Supervised learning
  - Unsupervised learning
- Disadvantages of deep learning for image registration  
(performance, # of training data, ground truth, ...)

