

Optimizing the NEXI acquisition protocol for human gray matter microstructure mapping on a clinical MRI scanner using Explainable AI

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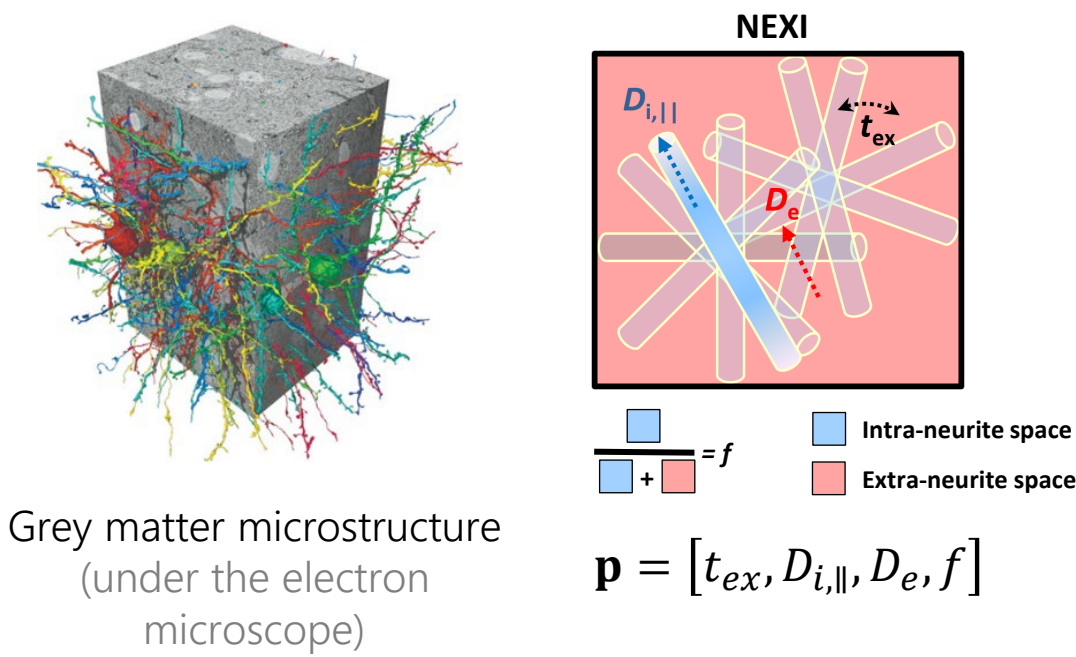


Declaration of Financial Interests or Relationships

Speaker Name: Quentin Uhl

I have no financial interests or relationships to disclose with regard to the subject matter of this presentation.

The Neurite Exchange Imaging model



- Geometry different from white matter
- Little myelin : water exchange across the cell membrane

From the parameters to the signal

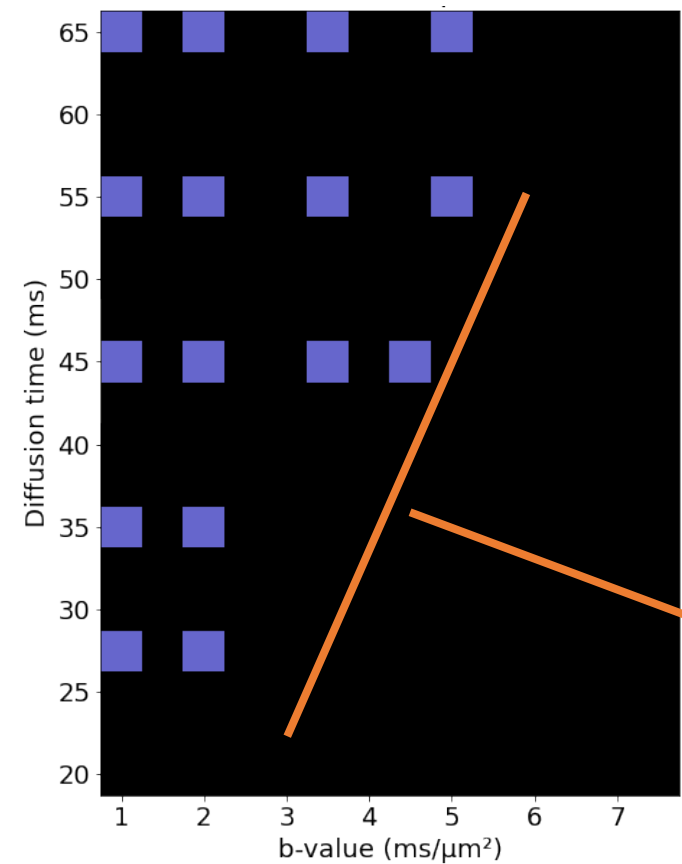
Kernel:	$\mathcal{K}(q, t, \mathbf{g} \cdot \mathbf{n}; f, D_{i, }, D_e, t_{ex}) = f' e^{-q^2 t D'_i} + (1 - f') e^{-q^2 t D'_e}$
Where: "apparent" diffusivities	$D'_{i/e} = \frac{1}{2} \left\{ D_{i, } (\mathbf{g} \cdot \mathbf{n})^2 + D_e + \frac{1}{q^2 t_{ex}} \mp \left[\left(D_e - D_{i, } (\mathbf{g} \cdot \mathbf{n})^2 + \frac{2f-1}{q^2 t_{ex}} \right)^2 + \frac{4f(1-f)}{q^4 t_{ex}^2} \right]^{\frac{1}{2}} \right\}$
"apparent" fraction	$f' = \frac{1}{D'_i - D'_e} [f D_{i, } (\mathbf{g} \cdot \mathbf{n})^2 + (1-f) D_e - D'_e]$
Powder average (over directions):	$\bar{S}(\mathbf{p}, q, t) = S \Big _{q=0} \cdot \int_0^1 \mathcal{K}(q, t, \mathbf{g} \cdot \mathbf{n}; \mathbf{p}) d(\mathbf{g} \cdot \mathbf{n})$

$$b = q^2 t = (\gamma G \delta)^2 t$$

→ Objective: retrieve \mathbf{p} from $\bar{S}(\mathbf{p}, b, t_d)$

multiple acquisition parameter combinations

Our MRI Protocol on the clinical 3T Prisma Scanner

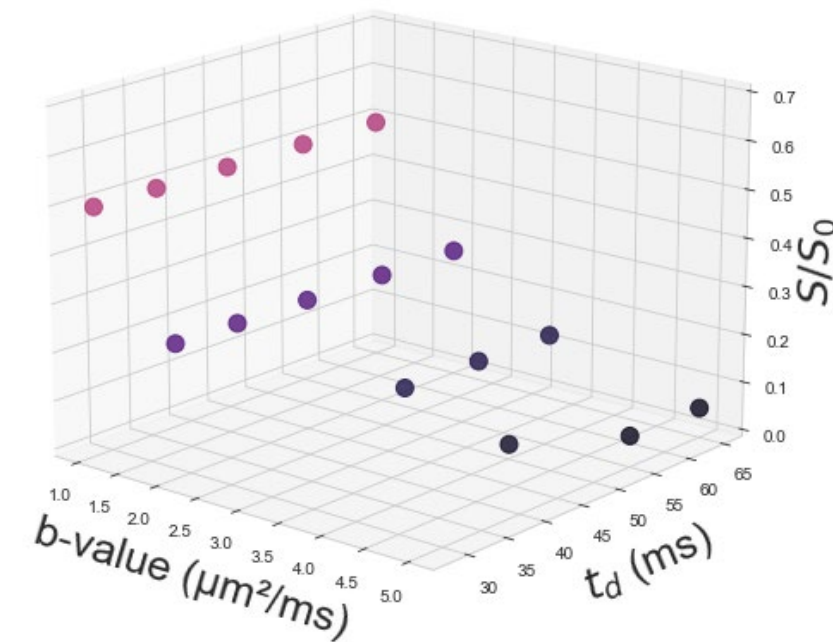


Additional information on the protocol

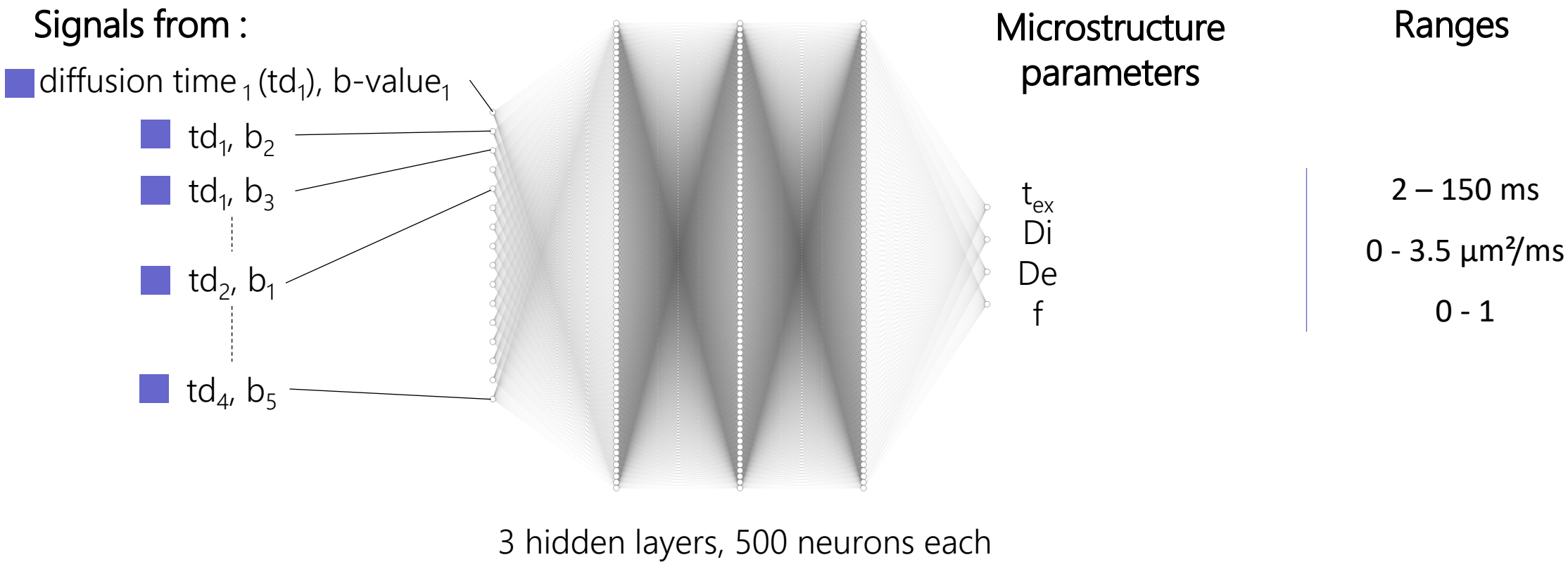
- Scan time: 35min
- Image resolution : 2x2x2 mm³
- Gradient duration : 16.5ms
- 20 directions per shell
- Echo time: 100ms

Gradient limitations (80mT/m)

Powder-averaged signal S depends on b and t_d



Retrieving parameters using a Multi-Layer Perceptron (MLP)

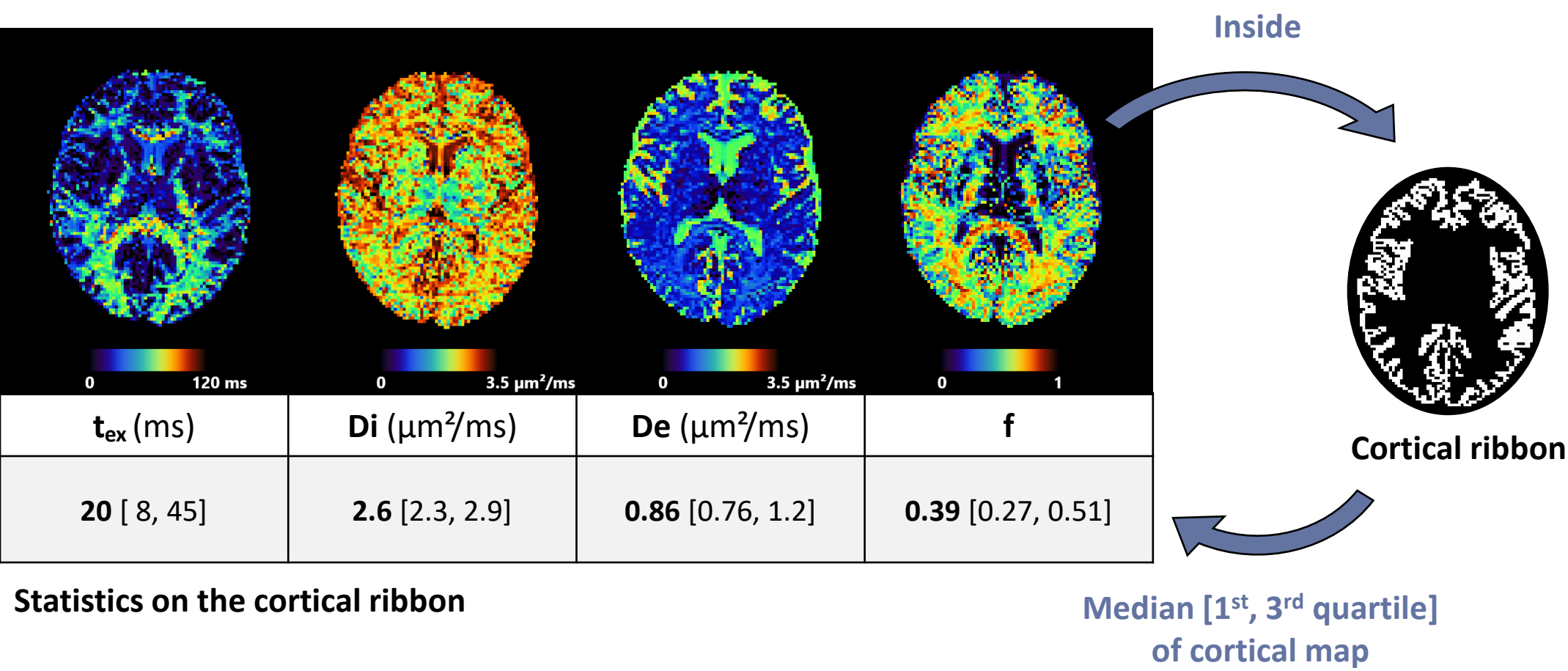


Retrieving parameters using a Multi-Layer Perceptron (MLP)

Training set : 2 000 000 examples
Test set : 10 000 examples
SNR : 80-120

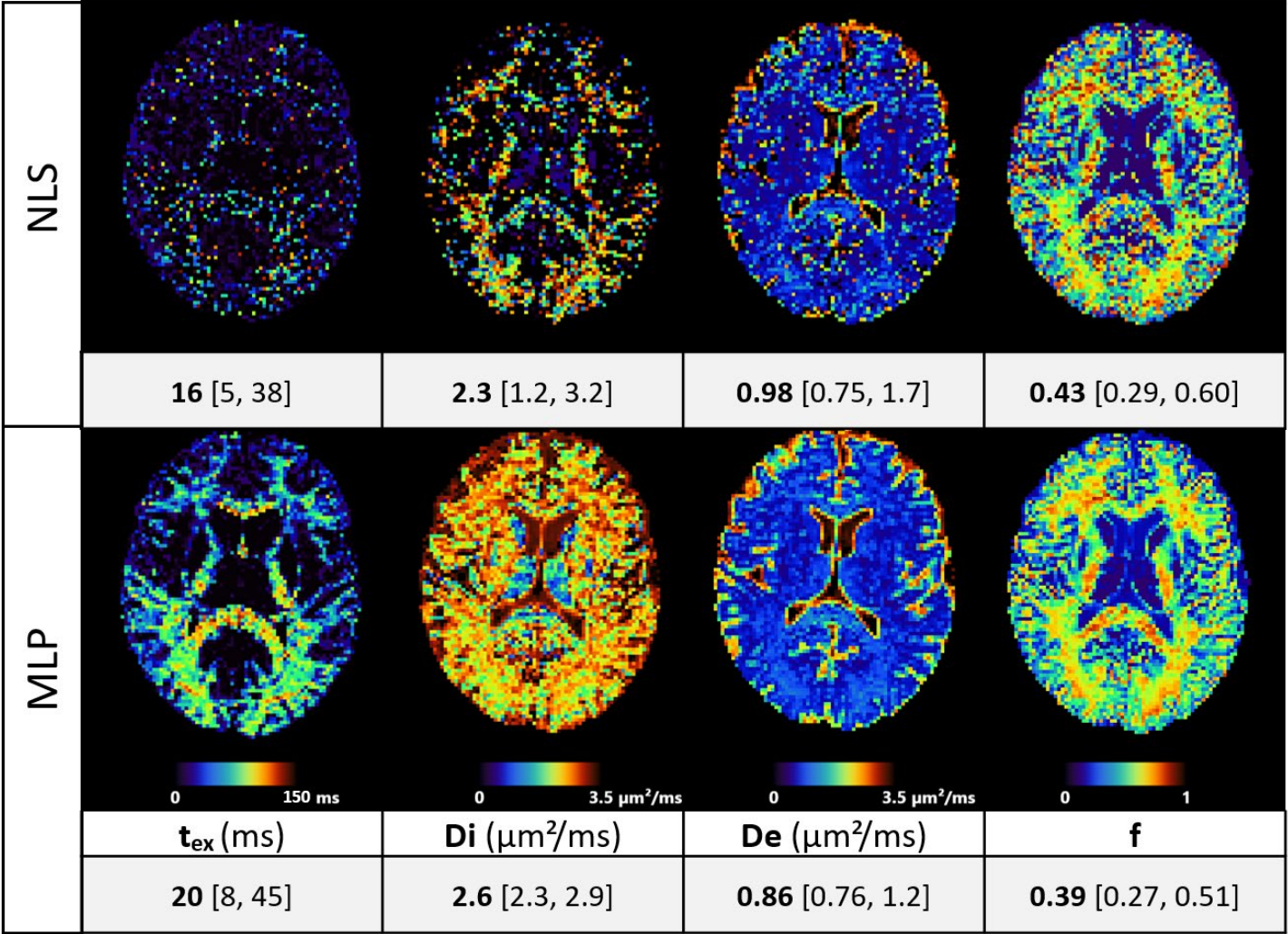
	t_{ex} (ms)	D_i ($\mu\text{m}^2/\text{ms}$)	D_e ($\mu\text{m}^2/\text{ms}$)	f
Clinical Protocol Mean Absolute Error (MAE)	27.457	0.423	0.351	0.083

MLP estimates on an axial slice of the human brain

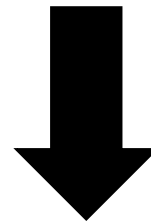


Statistics on the cortical ribbon

Comparison with the Non-linear Least Squares estimates



How to improve this protocol to get lower errors ?



Explainable AI

Shapley value of input i \sim its contribution to the output

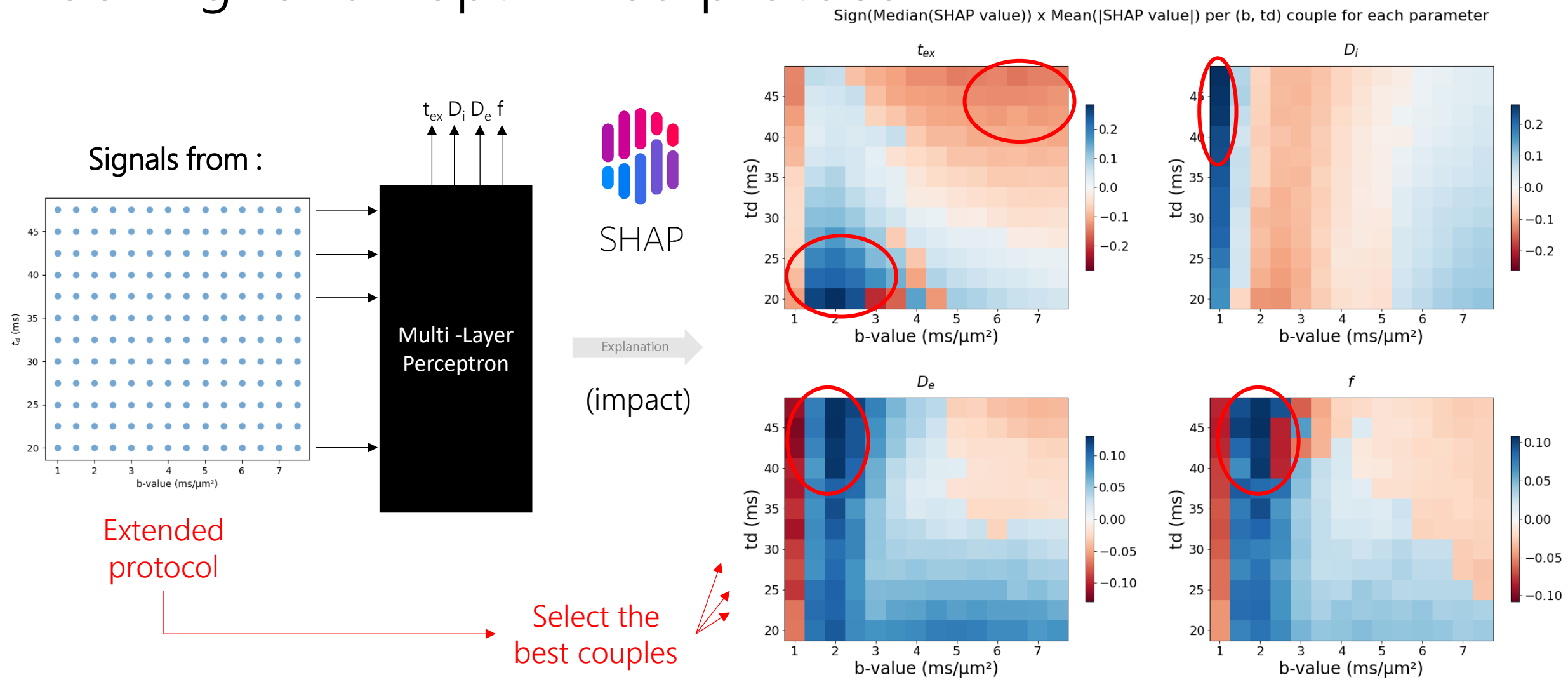
Explainable AI using Shapley values

Shapley value of player i ~ his/her contribution to the game:

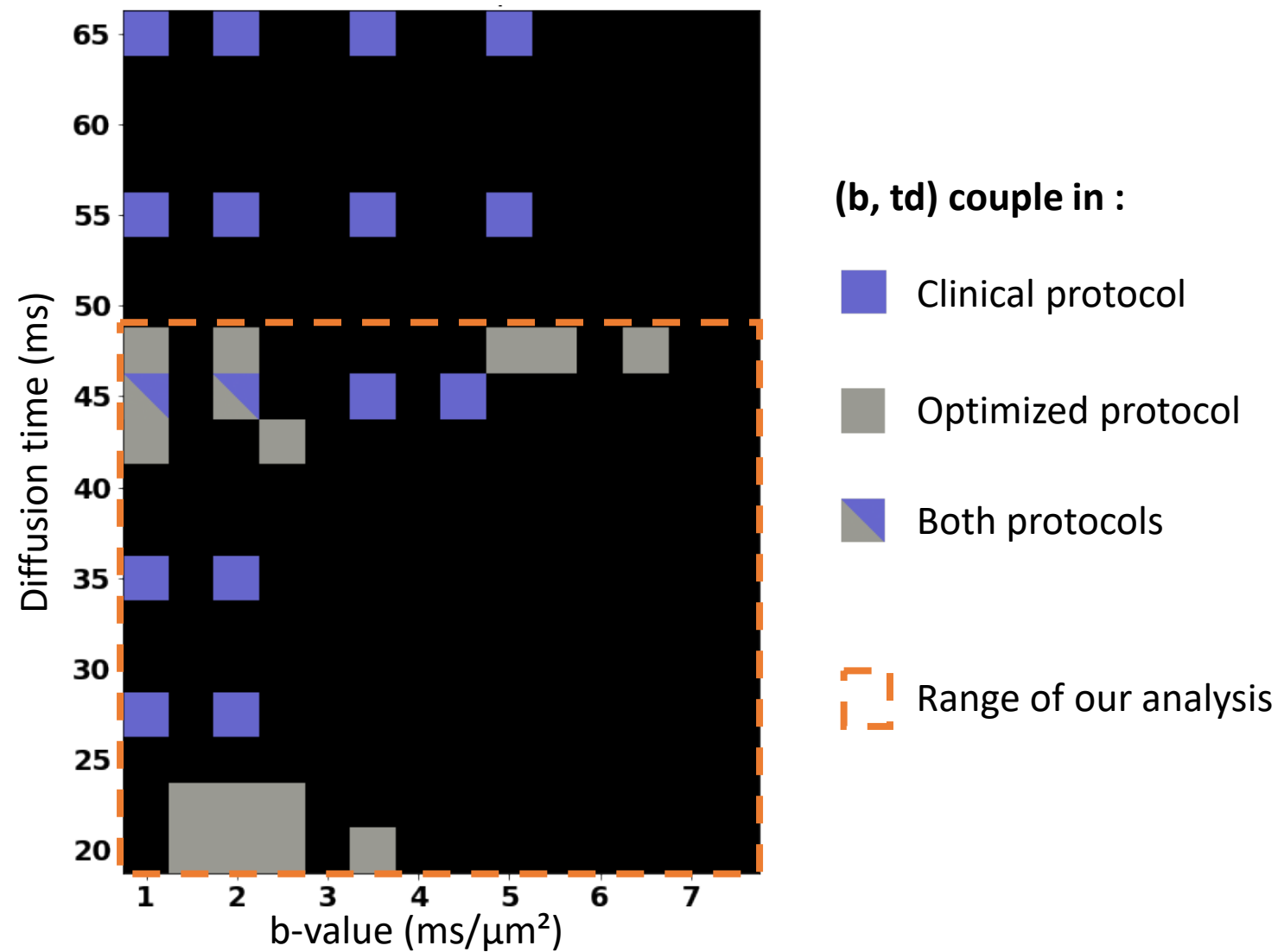
$$\varphi_i = \frac{1}{\# \text{ of players}} \sum_{\text{coalitions excluding } i} \frac{\text{marginal contribution of } i \text{ to coalition}}{\# \text{ of coalitions excluding } i \text{ of this size}}$$

the score of the team **with** the player
– the score of the team **without** the player

Looking for an optimized protocol



The two protocols



Is this new protocol really better ?

	t_{ex} (ms)	D_i ($\mu m^2/ms$)	D_e ($\mu m^2/ms$)	f
Clinical Protocol MAE	27.457	0.423	0.351	0.083
Optimized Protocol MAE	25.496	0.419	0.330	0.076
	-1.961	-0.004	-0.021	-0.007

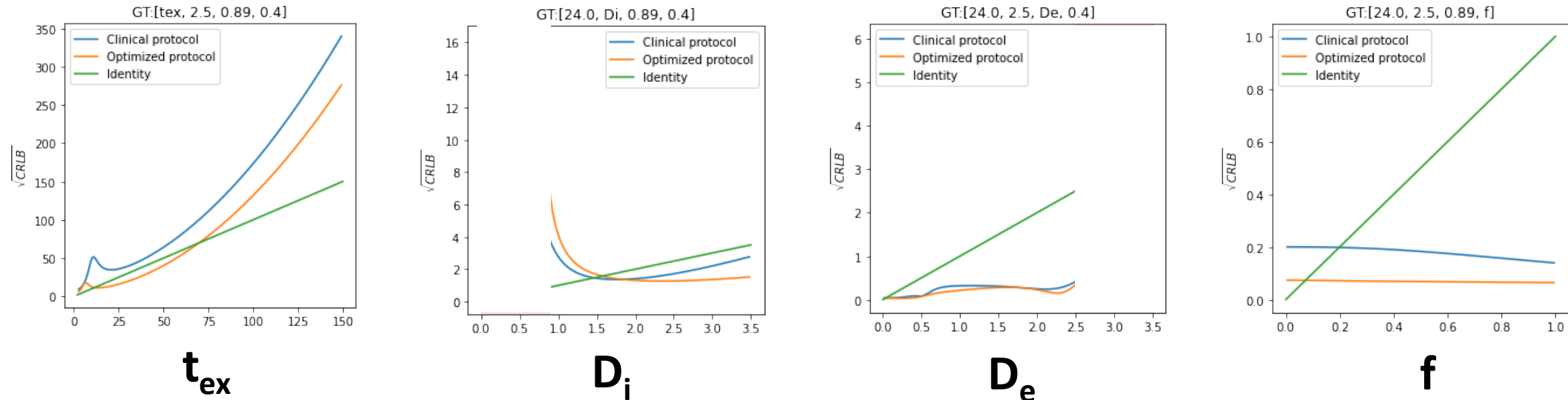
→ ⚠ Still dependent on the training & test sets

Is this new protocol really better ?

To compare protocols, we set side by side their associated **Cramer-Rao Lower Bound (CRLB)** on some sets of microstructure parameters.

⚠ Depends on the parameters \mathbf{p} (4D)

Around [24, 2.5, 0.89, 0.4]



Summary & Perspectives

- We succeeded in **estimating NEXI parameters on the human brain on a clinical scanner.**
- A **naïve protocol** seems to already hold **reasonable results.**
- Next, we will identify a new protocol **with this method** within a range adapted to the Prisma gradient limitations, **implement it** experimentally and **compare** the maps.

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