

# Low-field MRI's Spark on Implant Safety: A Closer Look at Radiofrequency Heating

Pia Sanpitak<sup>1</sup>, Bhumi Bhusal<sup>1</sup>, Jasmine Vu<sup>1,2</sup>, Laleh Golestanirad<sup>1,2</sup><sup>1</sup>Department of Radiology, Feinberg School of Medicine, Northwestern University <sup>2</sup>Department of Biomedical Engineering, McCormick School of Engineering, Northwestern University

## Introduction

- 2008 Report – 90% of the world lacked access to magnetic resonance imaging (MRI) [1]
- Low-field MRI scanners (0.55 T and below) – reduced cost, ease of siting [2]
- Are they “implant-friendly”?
  - Metal artifacts and risk of device dislodgment due to magnetic forces are reduced at lower fields
  - SAR tends to be lower at lower field strengths
  - Antenna Effect – SAR can be extremely high in the presence of elongated implants such as leads [3]
- Lack of quantitative data to support “implant-friendly” claims – needed to prevent unintended injuries
- Comparative study of power deposition in a tissue-mimicking gel around tips of implanted wires of different length and geometry during RF exposure at 23 MHz (0.55 T) compared to 64 MHz (1.5 T)

## Methods

### Systematic Simulations with Wire Models

- 368 Electromagnetic simulations in ANSYS Electronic Desktop 2021 R1 (ANSYS, Canonsburg, PA)
- Models of two 16-rung, high-pass, birdcage body coils tuned to their resonant frequencies (23 MHz – 0.55 T, 63.6 MHz – 1.5 T) (Figure 1A)
- Models of insulated and non insulated wires with apparent lengths varying from 10 cm to 120 cm at 5 cm intervals (Figure 1B-C)
  - Four different geometries for each wire: Straight and three different helical pitches
  - Wires were placed 15 mm from the edge, centered on the center axial plane of cylindrical tissue-mimicking phantom
  - Wire - platinum-iridium compound ( $\sigma = 4 \times 10^6 \text{ S/m}$ ,  $\epsilon_r = 1$ ), Insulation – Urethane ( $\sigma = 0 \text{ S/m}$ ,  $\epsilon_r = 3.5$ )
- Maximum of 0.1g-averaged SAR (0.1g MaxSAR) around the tip of each lead, input power of both coils adjusted to mean  $B_1^+$  of 2  $\mu\text{T}$  on central plane passing through coil’s iso-center (Figure 1D)

### Simulations with Realistic Deep Brain Stimulation (DBS) Lead Trajectories

- 2 patient models with implanted DBS leads – trajectories from post-operative computed tomography scans after surgery (Figure 2AB)
- Full DBS system: 40 cm lead + 60 cm extension + implantable pulse generator
- Lead-only system: 40 cm lead only
- Similar materials and SAR calculation as systematic simulations used for realistic simulations (Figure 2C)

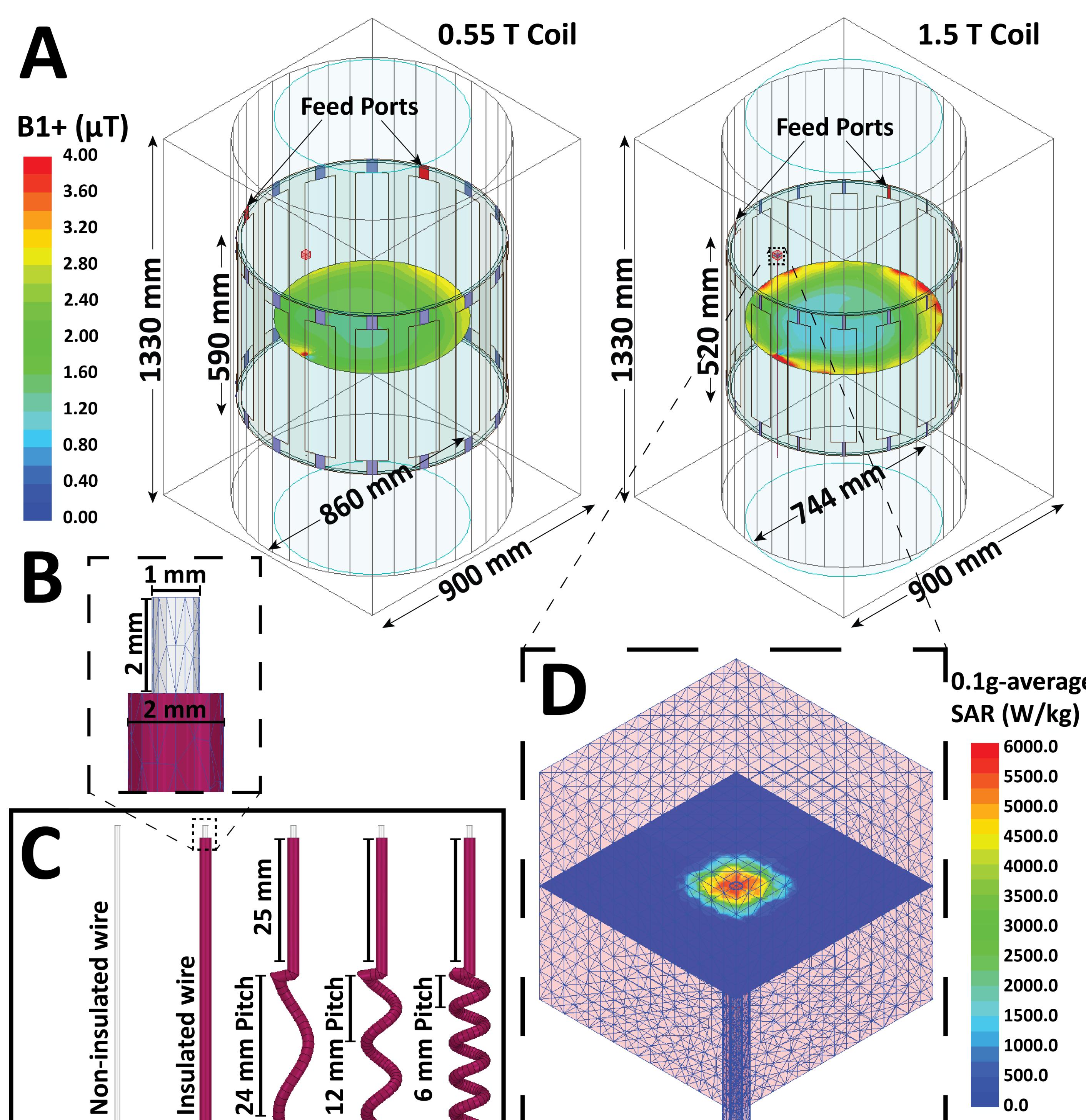


Figure 1. (A) Models of a 0.55 T and a 1.5 T birdcage coil loaded with a cylindrical phantom which contains a 75 cm straight insulated wire near the edge of the phantom. The input power of the coil is adjusted to generate  $B_1^+ = 2 \mu\text{T}$  at the iso-center. (B) A close view of the high-mesh area surrounding the wire and tip, and the high gradient SAR field in the tissue near the tip. (C) Display of different wire pitches.

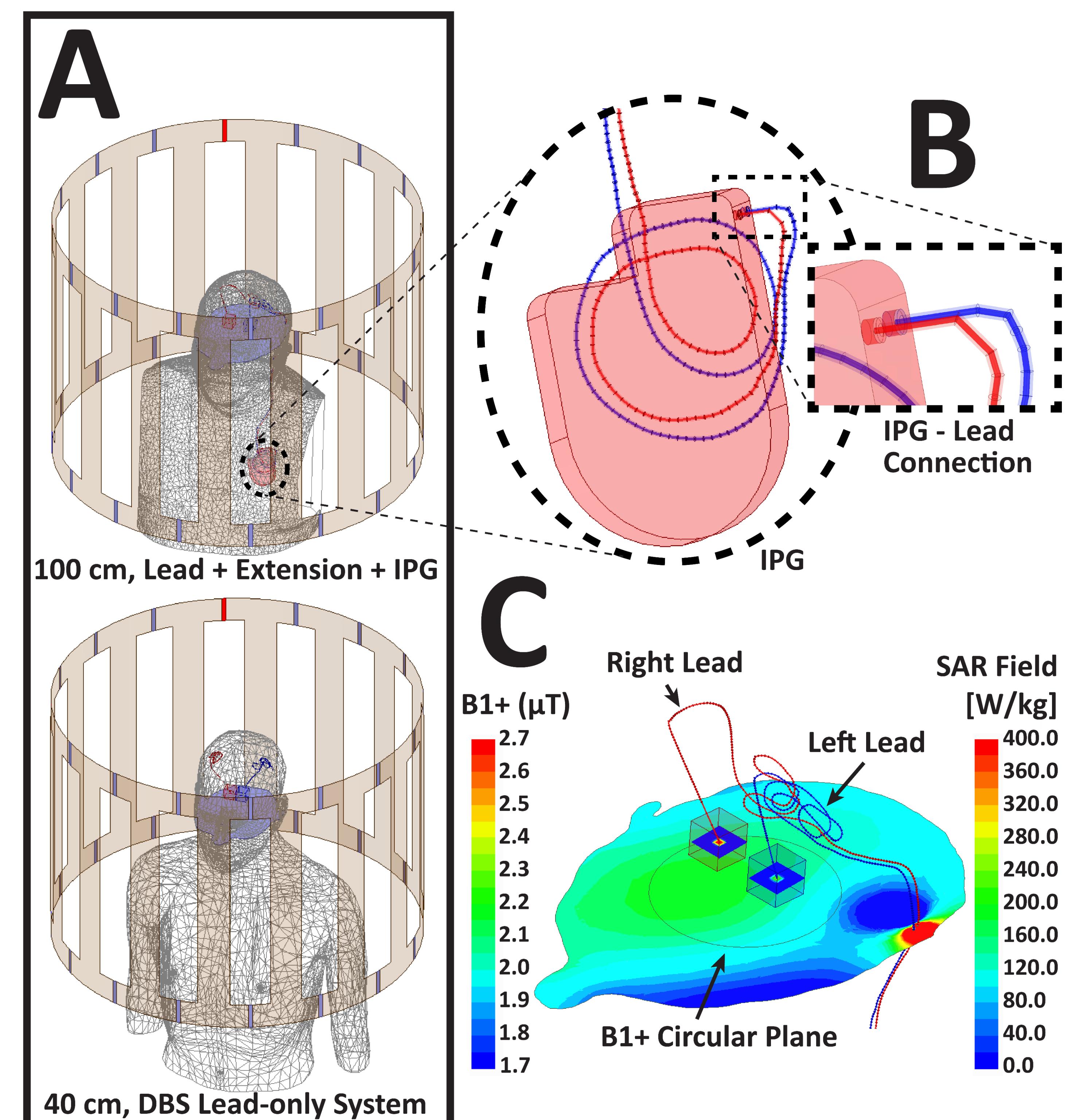


Figure 2. A) A DBS lead-only system with a 40 cm lead, and a full DBS system with a 40 cm lead connected to a 60 cm extension and a pulse generator (100 cm total length). B) Close view of the IPG-lead interface in the full system. C) Close up of the lead-only case the 1.5 T coil, showing the SAR fields near the tips of the leads and the  $B_1^+$  field on an axial slice located in the center of the coil.

## Results/Discussion

- Systematic Simulations – As the pitch decreases, apparent length where peak occurs gets shorter, and magnitude of peak 0.1g MaxSAR gets smaller (Figure 3A)
- DBS Simulations – 40 cm leads lower in 0.55 T than in 1.5, opposite for 100 cm (Figure 3B)
- Resonance effect – peaks occur when the length of the lead approaches the half-wavelength of RF wave in the medium [4]
- Serious ramifications in patients with long insulated leads, where the apparent length of the lead reaches 60+ cm, complicated internal geometries lead to even longer actual length
- 0.55 T scanners are not necessarily point-blank safer than 1.5 T scanners!

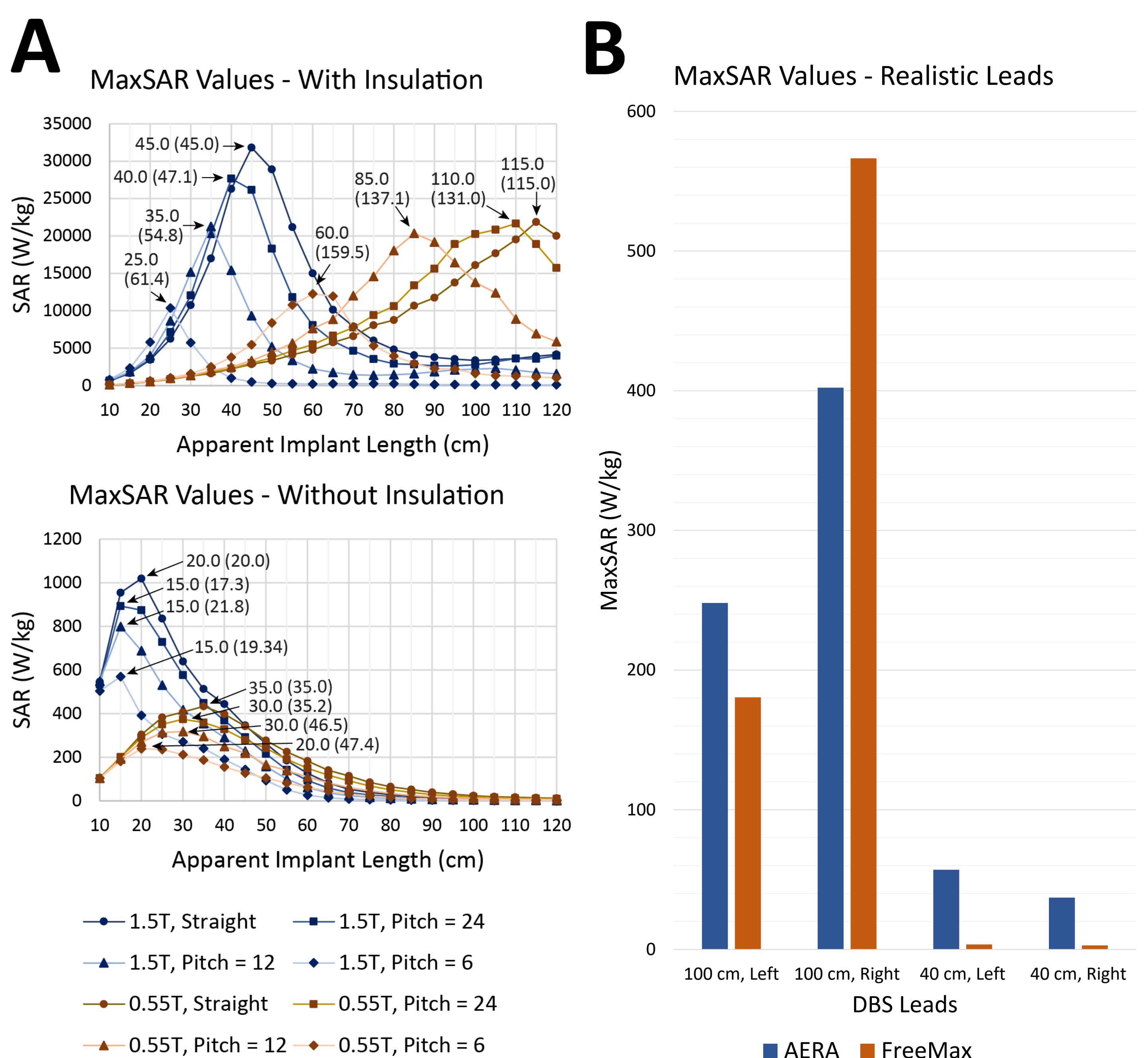


Figure 3. (A) 0.1g MaxSAR around tips of insulated and uninsulated wires in the 1.5 T and 0.55 T RF coils. For all simulations, the input power of the coil was adjusted to generate a mean  $B_1^+ = 2 \mu\text{T}$  on a central plane passing through the coil’s iso-center. The apparent and actual lengths (in parentheses) at which the peak occurred are denoted on the graphs. (B) Results of Realistic DBS implant simulations.