

## Research Article

# Supramolecular Self-Assembled Nanospheres for Enzyme Encapsulation Based on Cyclodextrin

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Based on the cyclodextrin (CD) and guest molecules inclusion, a novel rigid-flexible polymeric nanosphere was prepared by supramolecular self-assembly. The rigid part was formed by  $\alpha$ -cyclodextrin ( $\alpha$ -CD) and methoxypolyethylene glycol (mPEG) necklace-like crystallites while the flexible part was sodium alginate (Alg). The rigid and flexible parts were linked by  $\beta$ -cyclodextrin ( $\beta$ -CD) and ferrocene (Fc) inclusion complex. This kind of nanosphere exhibited good glucose oxidase (GOD) encapsulation ability. The encapsulated enzyme, in comparison to the free enzyme, is able to retain its high activities across a rather broader range of pH, temperature, and time. After 20 days, the encapsulated enzyme can retain its almost 86% initial activity which exhibited good storage stability. These studies suggested that CD host-guest inclusions to form stable polymeric nanospheres may be an effective way for enzyme encapsulation in various biomedical applications.

## 1. Introduction

In the past two decades, there has been a great deal of interest in supramolecular self-assembled polymeric microspheres due to their potential usages in drug encapsulation, transportation, and release areas [1–3]. As an intelligent and smart self-assembly, they can always change their aggregation state and structure to achieve certain physical or chemical performance and applications. For instance, they can be used as an ideal carrier for encapsulating large number of guest molecules or large-sized guests within the polymer's core domain [4, 5]. Furthermore, some can even respond to external stimuli like pH [6], light [7], temperature [8], specific molecules [9], and redox reactions [10].

Nowadays, the fabrication of a block copolymer is a common way to making polymeric microspheres [11, 12]. Kimura et al. have prepared a kind of block-pendant amphiphilic homopolymer which can selectively self-assemble into rod micelles or spheres by precisely adjusting the main chain length of this homopolymer [13]. Apart from the polymeric microspheres formed by the covalent bonded

amphiphilic block copolymers, noncovalently bonded microspheres based on supramolecular self-assembly have also been extensively studied [14–16]. Particularly, O'Reilly [17] and Weck's [18, 19] teams have introduced a preparing method called “block-copolymer-free.” In their approach, a kind of pseudo-copolymer has been prepared by self-assembling several kinds of homopolymers through supramolecular interaction. These homopolymers always connect with each other through weak bonds such as hydrogen bond,  $\pi$ - $\pi$  bond, and metal-ligand bond [20–22].

Cyclodextrins (CDs), as a kind of rather common supramolecules, are able to encapsulate a number of hydrophobic guest molecules and long-chained molecules such as adamantane, ferrocene, azobenzene, and PEG into their cavities to form stable hydrogen-bonded host-guest inclusion complexes [23–26]. CDs also have adjustable water solubility, excellent biocompatibility, and nontoxicity properties which are well suited as drug carriers for biomedical applications [27, 28].

In this paper, novel polymeric nanospheres, based on the “block-copolymer-free” strategy, have been prepared by

host-guest interactions of  $\beta$ -CD/Fc as well as  $\alpha$ -CD/mPEG. We firstly prepared  $\beta$ -CD modified sodium alginate (Alg- $\beta$ -CD) and ferrocene end-capped mPEG (mPEG-Fc) and further studied their host-guest self-assembly behavior in aqueous solution. As expected, this supramolecular copolymer linked by  $\beta$ -CD and Fc host-guest inclusions formed comb-shaped polymer in water. When  $\alpha$ -CD was added, the PEG long chain got through the cavities of  $\alpha$ -CDs and gradually formed the necklace-like crystalline inclusion. In this system, the mPEG/ $\alpha$ -CDs crystalline structure is the rigid section, while the hydrophilic sodium alginate serves as the flexible section, and the two sections were connected by Fc/ $\beta$ -CD inclusion complex. This specific rigid-flexible structure finally self-assembled into nanospheres in water. Further study showed that this kind of novel nanospheres exhibited high glucose oxidase (GOD) encapsulation efficiency and low GOD leakage efficiency and could also maintain high GOD activities over a rather broader pH and temperature range. These merits will benefit its application in a much wider field such as enzyme immobilization, microreactors, and drug delivery.

## 2. Experimental

**2.1. Materials.**  $\beta$ -CD,  $\alpha$ -CD, GOD, and glucose oxidase activity assay kit were purchased from Sigma. Methoxypolyethylene glycol (mPEG, Mw~5000) was bought from Shanghai Jingchunshiye Co., Ltd., China. Sodium alginate (Alg), carboxyferrocene (Fc-COOH), dicyclohexylcarbodiimide (DCC), morpholinoethanesulfonic acid (MES), 4-(dimethylamino)pyridine (DMAP), 1-ethyl-3-[3-(dimethylamino)propyl]carbodiimide hydrochloride (EDC), and N-hydroxysuccinimide (NHS) were acquired from Quzhou Laibo Co., Ltd., China.

### 2.2. Polymer Synthesis

**2.2.1. Preparation of the Alg- $\beta$ -CD.** Alg- $\beta$ -CD was prepared through two-step reactions. In the first step, mono-6-(p-tolylsulfonyl)- $\beta$ -cyclodextrin (6-CD-OTs) and mono-6-deoxy-6-hexamethylenediamine- $\beta$ -CD (6-CD-HDA) were synthesized following the procedures described in the previous literature [29, 30]. Subsequently, an amidation reaction involving amido and carboxyl group was employed to attach  $\beta$ -CD onto the Alg backbone. In short, 20 ml Alg with 1% concentration (w/v) was prepared in MES (0.1 M) and sodium chloride (0.5 M) buffer solution at pH = 6.0. After that, 190 mg EDC and 58 mg NHS (with a molar ratio of COO<sup>-</sup>: EDC: NHS = 1:1:0.5) were added to the Alg solution to activate the carboxylic acid groups on the polymer backbone. The solution was kept stirring for 30 min to achieve a uniform and clear solution. Subsequently, 40 mL of 6-CD-HDA MES solution was added and the reaction was conducted at 4°C for 12 h. The obtained mixture was dialysed in pure water for 4 days. The final product Alg- $\beta$ -CD was

obtained by freeze-drying. Equation (1) is used to calculate the degree of substitution (DS) of  $\beta$ -CD to Alg.

$$\frac{I_1}{I_2 - 6I_1 - 2/7I_1} = \frac{7}{4} \text{DS.} \quad (1)$$

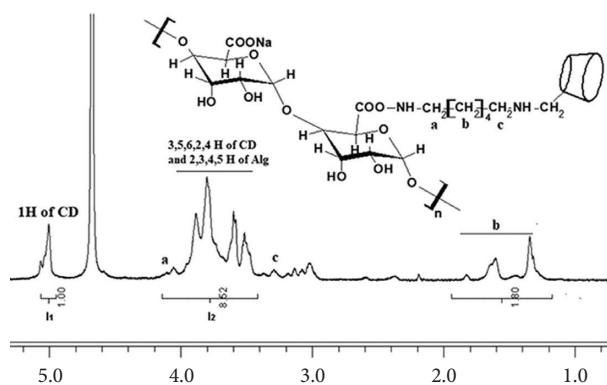
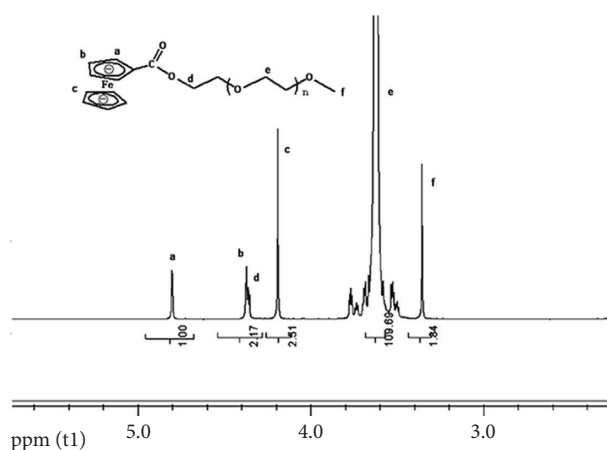
$I_1$  represents the digital integration of anomeric protons in  $\beta$ -CD, whereas  $I_2$  represents the overall digital integration between 3.4 and 4.2 ppm. The <sup>1</sup>HNMR of Alg- $\beta$ -CD in D<sub>2</sub>O (400 MHz) is presented in Figure 1 with a final DS of 25.6%.

**2.2.2. Preparation of the mPEG-Fc.** mPEG-Fc was synthesized with the one pot method [31, 32]. Carboxyferrocene (1.38 g) and mPEG (15.0 g) were dissolved in 200 ml dry CHCl<sub>3</sub>. Then DCC (2.24 g) and DMAP (0.366 g) were added successively and kept stirring for 24 h at room temperature. The mixture underwent filtration and rotary flash drying procedures at room temperature to remove the solvent CHCl<sub>3</sub> and byproduct dicyclohexylurea (DCU). The dried products were dissolved in deionized water and extracted with diethyl ether for three times. The lower layered product was gathered together and then passed through a gel column with methanol aqueous solution as solvent to further purify the target product mPEG-Fc from the remaining catalyst and carboxyferrocene residue. The final deep red product obtained was concentrated by spin drying and further dried with a vacuum oven for 2 days.

The integral ratio of  $H_d$  and  $H_f$  was used to calculate the DS of the final mPEG-Fc product. The <sup>1</sup>HNMR (400 MHz) of mPEG-Fc in CDCl<sub>3</sub> is shown in Figure 2, and the DS of mPEG-Fc calculated is 97.5%.

**2.3. Preparation of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD Nanospheres and Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD Nanospheres Loaded with GOD (Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD/GOD).** Alg- $\beta$ -CD (16.8 mg) and mPEG-Fc (52.5 mg) were added to 10 mL deionized water continuously and stirred for 3–5 hours until the product was fully dissolved. Following this,  $\alpha$ -CD (0.3 g) was added to the solution and kept stirring for 12 h. For GOD loading, 5.0 mg of GOD was added and stirred for 5 minutes before the addition of  $\alpha$ -CD. The solution changed from transparent to turbid gradually, indicating the formation of Alg- $\beta$ -CD/PEG-Fc/ $\alpha$ -CD and Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD/GOD nanospheres.

**2.4. Determination of GOD Encapsulation and Leakage Efficiency.** The encapsulation efficiency of GOD was measured in 50 ml aqueous solution with the GOD loading 0.5 mg and polymer concentration 0.5wt%. After the formation of polymer nanospheres, the suspension was subjected to centrifugal separation for 15 min at 12000rpm to separate the encapsulated and free GOD. The mass of free GOD was determined by measuring the supernatant using UV spectrophotometry.

FIGURE 1: The  $^1\text{H}$ NMR spectrum of Alg- $\beta$ -CD in  $\text{D}_2\text{O}$ .FIGURE 2:  $^1\text{H}$ NMR (400 MHz,  $\text{CDCl}_3$ ) spectrum of mPEG-Fc.

Equation (2) determines the encapsulation efficiency of the GOD.

$$\text{GOD of encapsulation efficiency (\%)} = \frac{\text{mass of GOD used in formulation} - \text{mass of free GOD}}{\text{mass of GOD used in formulation}} \times 100. \quad (2)$$

The above suspension was then stored at  $4^\circ\text{C}$  for 48 h to assess the GOD leakage efficiency. After that, the mixture was then subjected to centrifugal at 12000 rpm for 15 min to separate the encapsulated and free GOD.

Equation (3) determines the leakage efficiency of GOD.

$$\text{GOD leakage efficiency (\%)} = \frac{\text{mass of GOD used in the supernatant}}{\text{mass of GOD encapsulated}} \times 100. \quad (3)$$

**2.5. Activity of the Free and Encapsulated GOD.** It is known that the glucose and GOD can react to produce  $\text{H}_2\text{O}_2$  [33, 34]. Therefore, the  $\text{H}_2\text{O}_2$  production rate can be used to assess the activity of both free and encapsulated GOD.  $1\ \mu\text{M}$  GOD or encapsulated GOD was incubated at constant temperature in 50 ml phosphate or carbonate buffer

solutions with glucose concentration of 0.05 M for 30 min. The concentration of  $\text{H}_2\text{O}_2$  produced was determined by the glucose oxidase activity assay kit at OD 570 nm. And the relative activity of GOD is calculated by setting the optimal  $\text{H}_2\text{O}_2$  production as 100%, and results under other conditions should be scaled proportionally according to this.

**2.6. Measurement Method of the Michaelis Constant.** The Lineweaver–Burk plots were generated in a phosphate buffer with a pH of 7.0 at 25°C. To determine the kinetic parameters of both free GOD and encapsulated GOD, the values of  $K_m$  and  $V_{\max}$  were calculated by measuring the initial rates of glucose oxidation (0.11 to 2.11 mM), using a glucose oxidase concentration of 0.25 mg/mL. The data were plotted according to the Lineweaver–Burk double reciprocal model [35, 36] as follows:

$$\frac{1}{V} = \frac{k_m}{V_{\max}} \times \frac{1}{s} + \frac{1}{V_{\max}}, \quad (4)$$

where  $V$  and  $V_{\max}$  were the apparent initial catalytic rate and the maximum apparent initial catalytic rate, respectively.  $K_m$  refers to the apparent Michaelis constant and  $S$  represents the substrate concentration.

**2.7. Measurements.** The 2D  $^1\text{H}$ -NOESY NMR spectra were obtained using Bruker 600 NMR spectrometer at room temperature. High-resolution TEM was carried out by the JEM-2010 instrument with an accelerating voltage of 120 kV. AFM image was measured with a Bruker Multi-Mode 8 instrument in tapping mode. XRD was performed by X'Pert MPD with a scan rate of 2° theta/min in a Cu-K  $\alpha$  irradiation source.

### 3. Results and Discussion

Based on the previous report, it has been proved that Fc and  $\beta$ -CD as well as their derivatives can form inclusion complex spontaneously in aqueous solution [24]. In this paper, the 2D  $^1\text{H}$ -NOESY NMR spectra were also carried out to detect the mutual relations between the Fc groups on mPEG and  $\beta$ -CD groups on Alg. The resonance peaks at 3.7–4.0 ppm and 4.3–4.4 ppm can be attributed to the inner protons of  $\beta$ -CD and the protons of cyclopentadienyl ring in Fc, respectively. As shown in Figure 3, the hydrogen peaks of  $\beta$ -CD in Alg- $\beta$ -CD exhibited a clear correlation with the resonance of Fc in mPEG-Fc (the part circled by the red box), indicating that the Fc groups thrust into the inner cavity of  $\beta$ -CD groups and formed the inclusion complex. Similar results were also reported by other studies [37, 38].

The resulting Alg- $\beta$ -CD/mPEG-Fc was water-soluble transparent “graft copolymer.” By adding  $\alpha$ -CD to the Alg- $\beta$ -CD/mPEG-Fc homogeneous solution, the system gradually becomes turbid, suggesting some kind of aggregates had been formed in water. The morphology of these aggregates in the system was studied by high-resolution TEM and AFM equipment. Figure 4(a) shows the TEM image of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD aggregates; these aggregates showed round-line shapes with average diameters of around 80 nm. In the AFM image of Figure 4(b), the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD aggregates also showed round shape from the top view and appear to almost have the same diameters as the TEM image. Particularly, the height of these nanospheres was almost less than 5 nm which is about 15 times smaller than the lateral dimension. This can be attributed to the collapse of the nanospheres during

sample preparation. The same phenomenon was also reported by other studies [39, 40]. After encapsulated with GOD, as shown in Figure 4(d), the height of the nanospheres has a more than 5 fold increase compared with Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD unencapsulated nanoparticles, which indicates the successful encapsulation of GOD into the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanoparticles.

To further evaluate the structure of the CD-based inclusions, XRD is a commonly used method. Figure 5 shows the XRD patterns of  $\alpha$ -CD (Figure 5(a)), mPEG/ $\alpha$ -CD inclusion complex (Figure 5(b)), Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD (Figure 5(c)), and Alg- $\beta$ -CD and mPEG-Fc mixture (Figure 5(d)). The XRD pattern of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD demonstrated in the figure was quite different from that of free  $\alpha$ -CD, Alg- $\beta$ -CD, and mPEG-Fc mixture. The crystalline peaks of mPEG at  $2\theta = 19.2^\circ$  and  $23.3^\circ$  and  $\alpha$ -CD at  $2\theta = 21.5^\circ$  were absent [41, 42]. It can be also seen that the XRD pattern of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD was quite similar to that of mPEG- $\alpha$ -CD crystallites, both of which exhibited sharp peaks at  $2\theta = 19.9^\circ$ . According to the previous report [43–45], the peak appearing at  $2\theta = 19.9^\circ$  is a typical peak of mPEG- $\alpha$ -CD necklace-type crystallites which indicated that the inclusion structure of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD contained mPEG- $\alpha$ -CD crystallites. During the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanosphere formation process, water becomes a selective solvent for Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD. Insoluble mPEG- $\alpha$ -CD rigid part forms the inner core while the protonated coil-like Alg forms the outer shell. The zeta potential of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres measured was  $-28$  mV. This further confirms that the shell layer of the nanospheres is covered by negatively charged protonated Alg.

Based on the discussion above, the possible mechanism of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres' self-assembly processes is shown in Figure 6. Firstly, when the Alg- $\beta$ -CD and mPEG-Fc are dissolved in water together, the  $\beta$ -CD group will form inclusion complex with Fc group to get a pseudo-graft copolymer Alg- $\beta$ -CD/mPEG-Fc. After  $\alpha$ -CD was added to the solution and stirred for several hours, the branched mPEG part of Alg- $\beta$ -CD/mPEG-Fc would thread through the  $\alpha$ -CDs' inner cavity one by one and finally form the necklace-type crystalline structure. These crystallites are rigid and insoluble in water which incline to gather together to form the hydrophobic core, while the coil-like hydrophilic Alg part will form the outer shell. Through these self-assembly processes, the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres finally formed. Particularly, when the enzyme was added at this process, it will be partly encapsulated into the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres.

In fact, these Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres have shown excellent GOD encapsulation capacity. According to the measuring method introduced in Section 2.4, the GOD encapsulation and leakage efficiency calculated were 68.5% and 6.4%, respectively, which indicate that these nanospheres have great potential in drug delivery systems for medical application.

To further investigate the binding ability of GOD and Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres after encapsulation, the

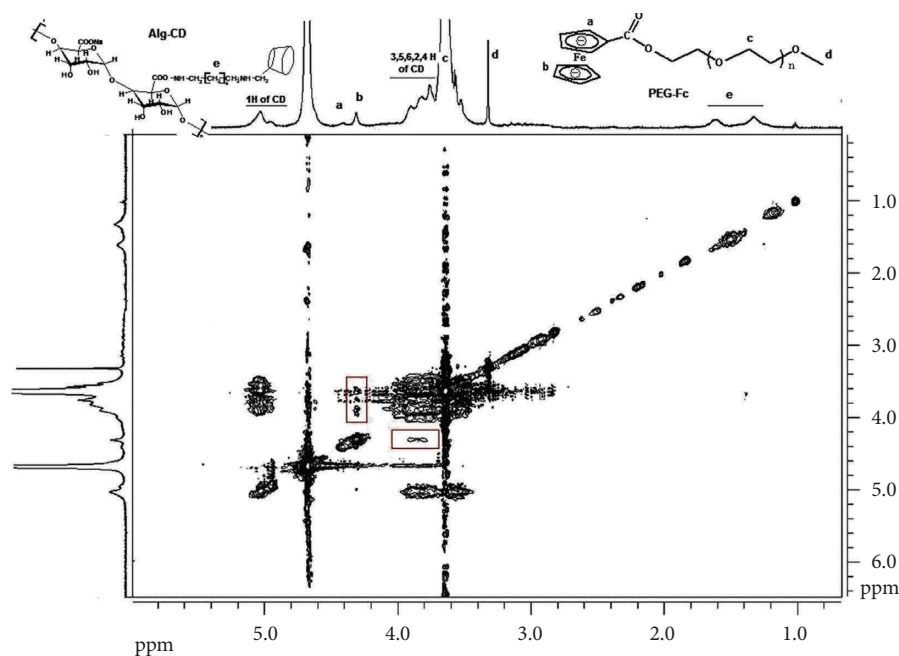


FIGURE 3: 2D  $^1\text{H}$ -NOESY NMR spectrum of a mixture of mPEG-Fc and Alg- $\beta$ -CD ICs in  $\text{D}_2\text{O}$ .

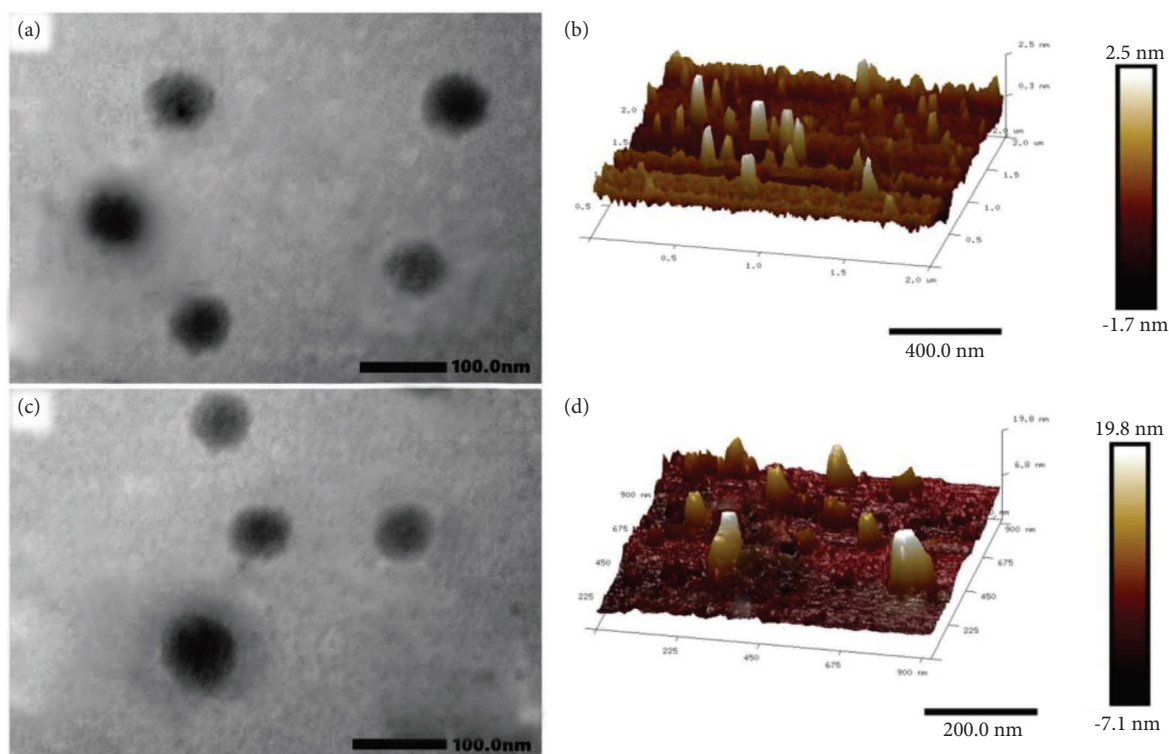


FIGURE 4: (a) The TEM image of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres. (b) The AFM image of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres. (c) The TEM image of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres encapsulated GOD. (d) The AFM image of Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres encapsulated GOD.

Michaelis constant was determined. The Lineweaver–Burk double reciprocal plots of free and encapsulated GOD are demonstrated in Figure 7. The liner equations obtained were  $y = 8.711x + 2.297$  and  $y = 10.621x + 1.731$ ,

respectively. The Michaelis constant ( $K_m$ ) of encapsulated GOD ( $3.79 \times 10^{-3} \text{ M}$ ) in nanoparticles was much lower than that of free GOD ( $6.14 \times 10^{-3} \text{ M}$ ), which indicates that the affinity between GOD and its substrate

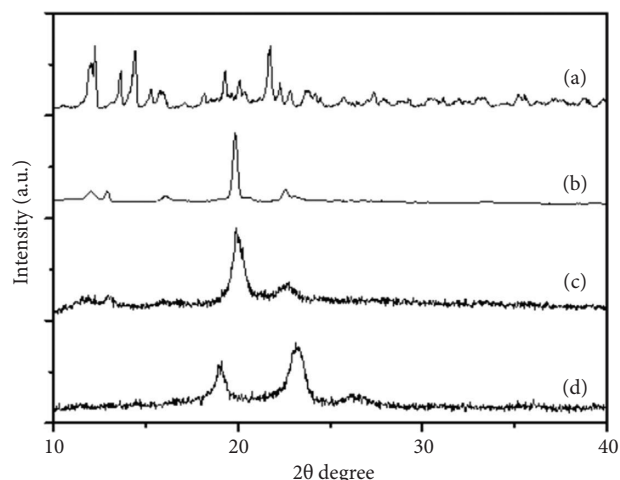


FIGURE 5: X-ray diffraction patterns of (a)  $\alpha$ -CD, (b) mPEG/ $\alpha$ -CD inclusion complex, (c) Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD particles, and (d) Alg- $\beta$ -CD and PEG-Fc mixture.

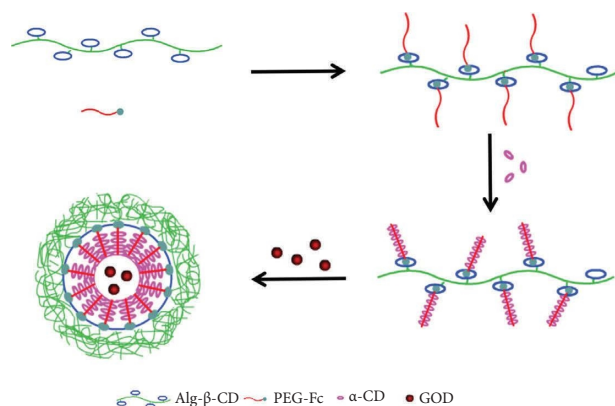


FIGURE 6: The mechanism of the self-assembly processes of Alg- $\beta$ -CD/PEG-Fc/ $\alpha$ -CD nanospheres encapsulated GOD.

has increased after the GOD encapsulated in the Alg- $\beta$ -CD/PEG-Fc/ $\alpha$ -CD nanospheres.

The impact of pH on the activities of both free and encapsulated GOD was assessed at 25°C over a pH range from 3 to 10. The free GOD, as illustrated in Figure 8, demonstrated peak relative activity at pH = 6.0. In comparison, the encapsulated GOD demonstrated high relative activities in a rather wide pH range from 5.0 to 7.0. The possible reason is the aggregation effect of GOD molecules which gathered in a rather small core. The three-dimensional structure of the encapsulated GOD is rather difficult to change and their pH stability greatly improved. This result indicates that the Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD nanospheres could stabilize the GOD activity over a much broader pH range, which will benefit its medical application.

The effect of temperature on free and encapsulated GOD activities was measured in a water thermal bath at the constant temperature from 15 to 75°C. As illustrated in Figure 9, both the free and encapsulated GOD showed maximum relative activities at about 45°C. But the

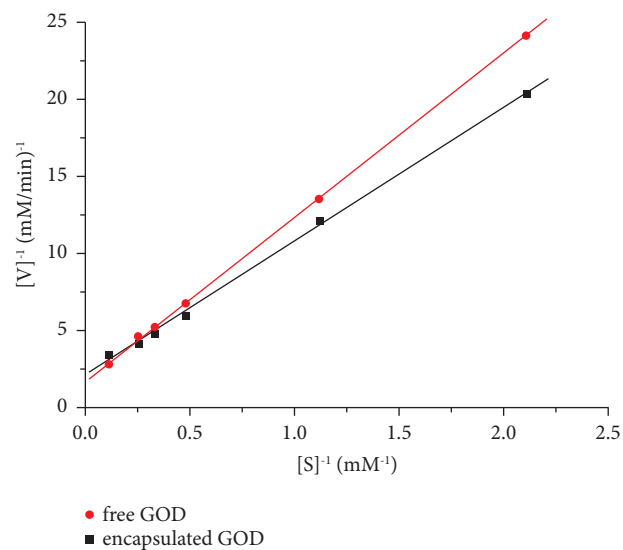


FIGURE 7: The Lineweaver-Burk plots of free GOD and encapsulated GOD in the nanospheres.

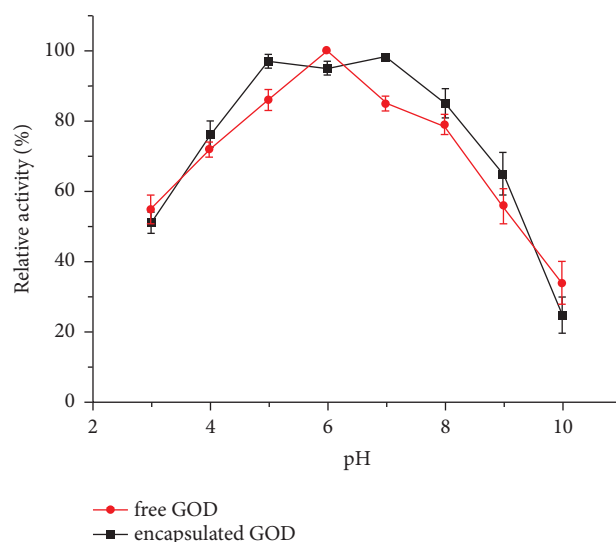


FIGURE 8: The impact of pH on the activities of both free GOD and encapsulated GOD.

encapsulated GOD could keep rather high relative activities at a broad temperature range from 35 to 55°C, while for the free GOD, there was an obvious decrease before and after the optimum temperature at this temperature range. When the temperature exceeds 55°C, the relative activities for both free and encapsulated GOD showed a significant downward trend with the increasing temperature. These results indicate that the Alg- $\beta$ -CD/PEG-Fc/ $\alpha$ -CD nanospheres could stabilize the GOD activities at a broad temperature range.

Long-term stability is a very important indicator for encapsulated enzymes in most application scenarios. The storage stability of free and encapsulated GOD was investigated in 0.2 M acetate buffer (pH 6.0) at 4°C for 20 days. As shown in Figure 10, in the beginning 5 days, encapsulated GOD maintained as high as 98% relative activity.



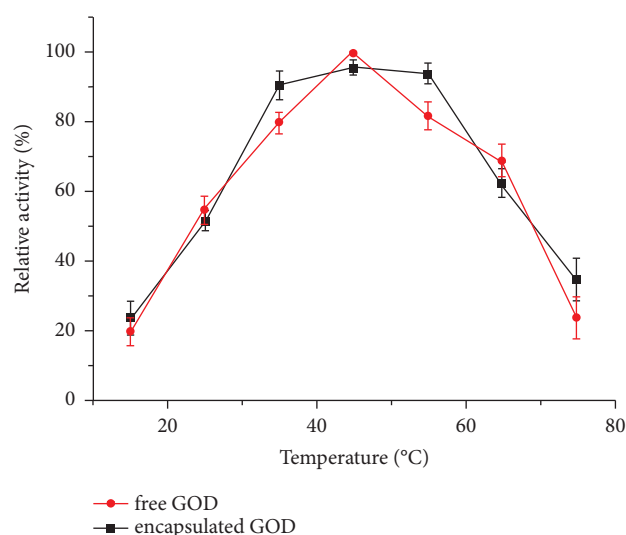


FIGURE 9: The impact of temperature on the activities of both free GOD and encapsulated GOD.

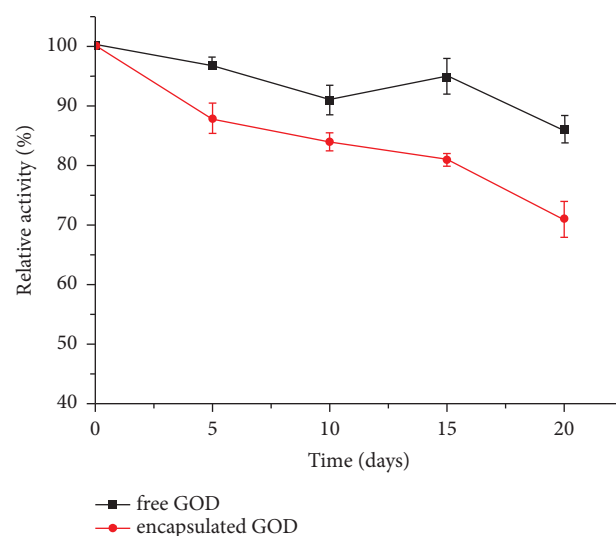


FIGURE 10: Storage stability of the free GOD and encapsulated GOD.

In comparison, free GOD retained only 88% relative activity. Even after 20 days, the encapsulated GOD exhibited almost 86% of its initial activity while for free GOD, there was only 71% relative activity left. These results indicate that the Alg- $\beta$ -CD/PEG-Fc/ $\alpha$ -CD encapsulation methods reported in this paper could significantly improve the storage stability of GOD.

#### 4. Conclusion

To summarize, based on the self-assembly of  $\beta$ -CD/Fc and mPEG/ $\alpha$ -CD inclusions, Alg- $\beta$ -CD/mPEG-Fc/ $\alpha$ -CD rigid-flexible nanospheres were successfully prepared as novel carriers for GOD encapsulation. Although being encapsulated into nanospheres, GOD still maintains high activity, and the affinity between the encapsulated GOD and substrate has been slightly enhanced. Additionally, the encapsulation of GOD expanded the optimal pH and temperature

ranges for the enzyme's activity and meanwhile improved GOD's storage stability. We believe that the encapsulation methods described in this study present a strategy for maintaining the biological functionality of protein-based pharmaceuticals in medical use.

#### Data Availability

All the data used in this study are included within the article.

#### Conflicts of Interest

The authors declare that they have no conflicts of interest.

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