

# [Re] Chemical Signalling in the Neurovascular Unit

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## Competing Interests:

The authors have declared that no competing interests exist.

 [Article repository](#)

 [Code repository](#)

 [Data repository](#)

## A reference implementation of

→ Witthoft A, Karniadakis GE (2012) A bidirectional model for communication in the neurovascular unit. *Journal of Theoretical Biology* 311: 80-93.

## Introduction

Witthoft and Karniadakis [1] introduced a model for communication via chemical signalling within the neurovascular unit (NVU). In the NVU neurons communicate their nutrient requirements to the cerebral arteries via astrocytes [3]: the activity of neurons releases glutamate and potassium into the synaptic space, causing astrocytes to release potassium into the periarterial space via their end-feet, leading to the activation of smooth muscle cells in the artery wall and thus a dilation of the artery to increase blood flow.

Functional hyperemia is an important mechanism in the brain, by which an increased neuronal metabolism leads to an increase of blood flow in surrounding arteries in order to maintain adequate oxygen and nutrient supply to the active neurons. This process works via a cascade of chemical signalling processes from neurons to astrocytes to arteries. The unidirectional vascular response to increased neuronal demands has previously been modelled [6][4], however, these models did not include the activity of the transient receptor potential vanilloid-related channel 4 (TRPV4). The TRPV4 channel is a mechanosensitive calcium channel and leads to a depolarisation of the astrocyte in response to the dilation of the artery wall.

The paper contains the differential equations that are being modelled, however no code repository is provided. The model is useful for the investigation of the effect of cerebrovascular diseases on the brain and thus an openly available code repository reproducing the results of this paper will be helpful to other researchers.

## Methods

The paper indicates that the original code was written in Matlab, while the reproduction presented here is written in Python 3.5. The model is given as a series of ordinary differential equations (ODE), which are implemented as a function `nvu()`. This function is solved using the `scipy.integrate` library. Initial attempts to solve the system of ODE using the standard function `odeint()` failed. Instead, the equations can be solved using the function `ode()` with the integration method set to “lsoda”, which automatically selects between the Adams method for non-stiff and BDF for stiff problems. The ODE system described in [1] is a stiff system. Values for absolute and relative tolerance have to be set in order for the simulation to finish successfully.

These are given in the results section as they differ for different simulations. Future users of this code should note that the simulation of a longer time span may require the use of different values for absolute and relative tolerance, which have to be found via trial and error, but from experience, they should not be larger than  $1e-4$  or smaller than  $1e-11$ .

The code was implemented following the descriptions of the equations in [1], but upon cross-checking equations against their equivalents in [6][4][5] it became evident that some of the equations contain typographical errors. This was confirmed after contacting the authors of [1]. Changes to the equations are as follows:

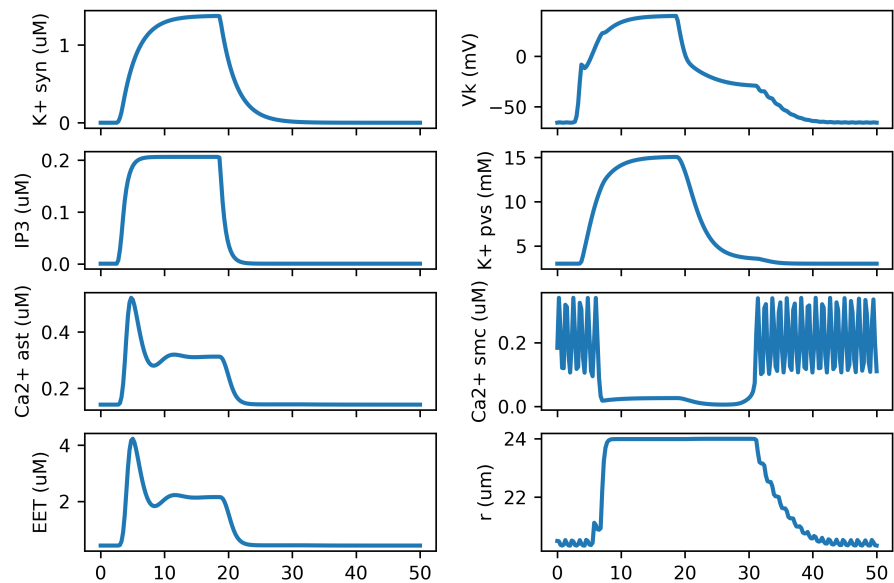
- $I_{\Sigma K}$  in (20) should be defined as  $I_{\Sigma K} = -J_{\Sigma K}C_{astr}\gamma$  (changed sign).
- (23)  $J_{Ca}$  is not defined in the manuscript, but correspondence with the original authors revealed that it should be defined as  $J_{Ca} = -I_{Ca}/(C_{SMC}\gamma)$ .
- (31)  $I_K = g_K n(V_m - v_K)$  [4].
- (A.1) Term  $\frac{1}{2\alpha}I_{Ca}$  should be  $\alpha I_{Ca}$  (to comply with code for [2] by the original authors).
- (A.3) When implementing this equation it has to be multiplied by  $\mu m$  to get the correct units of force.
- (A.6) The brackets around the exponential function are set incorrectly, it should read  $\exp\left(\frac{-(y'-y'_0)^2}{2[y'_1/(y'+y'_2)]^{2y'_4}}\right) - y'_3$  [5].
- Parameter  $C_{SMC}$  is given as  $C$  in Table B2
- Decimal of parameter  $a$  in Table B2 is in the wrong place, it should read  $a = 502.65 \mu m^2$
- The value for  $[Ca^{2+}]_{ER}$  is not given, but can be found in [6] as  $[Ca^{2+}]_{ER} = 400\mu m$
- Parameter  $k_{Ca} = 1.3568e2 \text{ nM/C}$  is incorrectly cited from [5]

Furthermore, upon correspondence with the original authors, an equilibration phase of 20 s before the simulation had to be implemented. During the equilibration phase no glutamate or potassium is released into the synaptic space and the solution values at the end of the equilibration phase is used as initial values for the main simulation. This step is not mentioned in the original publication, but is vital to obtain the correct results.

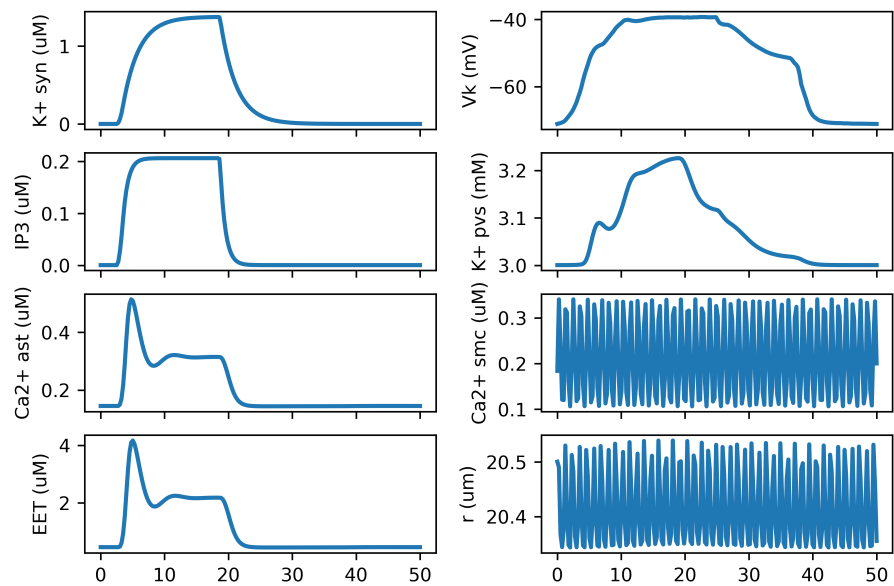
## Results

Results from the code presented in this repository aim at reproducing Figure 5 in the original application, which shows ion and voltage dynamics over a simulation period of 50 s.

Figure 1 shows the results obtained from the code in this repository. Potassium ( $K^+$ ) in both the synaptic and perivascular space match their corresponding plots in the original publication, as do calcium ( $Ca^{2+}$ ) in the smooth muscle cell and the arterial radius. Differences can be seen for  $Ca^{2+}$  in the astrocyte, EET and the astrocyte membrane potential  $V_k$ . In the case of astrocytic  $Ca^{2+}$  and EET the first peak overshoots compared to the results in the original publication, while the remainder of the plots match the original publication. Most interesting is the shape of  $V_k$ , which in the first half looks very different from the reproduced figure. Additionally,  $V_k$  overshoots into positive values, which is not given in the original publication. Simulation tolerance values were  $atol=1e-7$  and  $rtol=1e-7$ .



**Figure 1:** Astrocyte and arterial response during neuronal stimulation. This figure is a reproduction of Figure 5 in the original publication using the code in this repository. Potassium ( $K^+$ ) in both the synaptic and perivascular space match their corresponding plots in the original publication, as do calcium ( $Ca^{2+}$ ) in the smooth muscle cell and the arterial radius. Differences can be seen for  $Ca^{2+}$  in the astrocyte, EET and the astrocyte membrane potential  $V_k$ . In the case of astrocytic  $Ca^{2+}$  and EET the first peak overshoots compared to the results in the original publication, while the remainder of the plots match the original publication. Most interesting is the shape of  $V_k$ , which in the first half looks very different from the reproduced figure. Additionally,  $V_k$  overshoots into positive values, which is not given in the original publication. Simulation tolerance values  $atol=1e-7$ ,  $rtol=1e-7$ .



**Figure 2:** Astrocyte and arterial response during neuronal stimulation whilst  $V_k$  is fixed to match the original publication. The difference in results for  $K^+$  in the perivascular space,  $Ca^{2+}$  in the smooth muscle cell and arterial radius suggest that possible further errors in the equations exist in the original publication. Simulation tolerance values  $atol=1e-7$ ,  $rtol=1e-7$ .

The large difference in  $V_k$  between the two simulations is surprising, especially because this does not lead to incorrect results in the other plots, apart from an overshoot of the values for  $Ca^{2+}$  and EET in the astrocyte. The key results, which are the response of  $Ca^{2+}$  and subsequently the arterial radius match the original publication. A newer publication by the same authors exists [2], which does contain the same spike for  $Ca^{2+}$  and EET as the simulation results presented here. It is unclear, where this difference comes from as [6] does not indicate that any of the equations affecting  $Ca^{2+}$  or EET have been altered. It is also unclear why  $V_k$  shows such a large difference.

One possible explanation could be that some components of  $\partial V_k / \partial t$  are wrongly implemented, but the results are mostly affected by the mere fact that  $V_k$  increases in response to the stimulus instead of the exact value of  $V_k$ . To test this,  $V_k$  was obtained from the original publication and hard-coded into the simulation instead of being calculated from its ODE. This is shown in Figure 2. Simulation tolerance values were  $atol=1e-7$  and  $rtol=1e-7$ . Here, the results for  $K^+$  in the perivascular space,  $Ca^{2+}$  in the smooth muscle cells and the arterial radius differ largely from the results in the original publication or indeed Figure 1. Because of this discrepancy between results the authors of the original publication were contacted to request the code for this publication. However, they could only provide the Matlab code for [2], from which it was not possible to revert back to the code to implement [1]. Attempts were made to remove the additional equations introduced in [2] from this code in order to revert it back to what it might have been at the time of publication of [1]. However, the results did not match. The original authors were asked for advice, but stated that it would likely be impossible to revert the code back to its original version due to the sensitivity of parameters, which would make this processes immensely error prone.

## Conclusion

To a large degree the results from [1] were replicated. However, distinct differences in the results remain, which could not be explained. It should be emphasised that the

number of errors found in the original publication may indicate that more errors may remain to be found, however, because no version of the code to implement [1] appears to exist anymore, it will be very difficult at best to find these additional errors.

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