

Inducing Vertebrate Limb Regeneration: A Review of Past Advances and Future Outlook

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Limb loss due to traumatic injury or amputation is a major biomedical burden. Many vertebrates exhibit the ability to form and pattern normal limbs during embryogenesis from amorphous clusters of precursor cells, hinting that this process could perhaps be activated later in life to rebuild missing or damaged limbs. Indeed, some animals, such as salamanders, are proficient regenerators of limbs throughout their life span. Thus, research over the last century has sought to stimulate regeneration in species that do not normally regenerate their appendages. Importantly, these efforts are not only a vital aspect of regenerative medicine, but also have fundamental implications for understanding evolution and the cellular control of growth and form throughout the body. Here we review major recent advances in augmenting limb regeneration, summarizing the degree of success that has been achieved to date in frog and mammalian models using genetic, biochemical, and bioelectrical interventions. While the degree of whole limb repair in rodent models has been modest to date, a number of new technologies and approaches comprise an exciting near-term road map for basic and clinical progress in regeneration.

Patients who lose limbs to injury, cancer, or degenerative diseases must readjust nearly every aspect of their lives. The most recent study aiming to quantify limb loss in the United States found that, as of 2005, there are 1.6 million individuals living with limb loss, with the number of amputees increasing by 185,000 each year to a projected 3.5 million by 2050 (Ziegler-Graham et al. 2008). Besides the unquantifiable suffering it imposes, limb loss presents life-long challenges, some of which currently have no adequate solution. Although inorganic prosthetics are improving (Windrich et al. 2016; Trent et al. 2020), organic restoration of a lost appendage would be the definitive solution. While great

progress has been made in methods to treat superficial wounds resulting in rapid, nearly scarless healing (Moore et al. 2018; Monavarian et al. 2019), complete renewal of vertebrate limbs remains a fundamental challenge to overcome. Because most vertebrates create perfect limbs during embryogenesis, it is clear that their genomes and cellular pathways possess the information needed to create the needed anatomical structures. Could this information be reaccessed during adulthood in cases of traumatic injury or disease-induced amputation?

Appendage regeneration is not only a profound unmet biomedical need. It is also a paradigm case of a more fundamental problem of

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D. Davidian and M. Levin

evolutionary, developmental, and synthetic biology: how do cells cooperate to build specific complex organs and stop precisely when the correct anatomical structure is complete (Pezzulo and Levin 2016)? How are cellular collectives driven to build one structure rather than another from exactly the same cellular building blocks (e.g., hand vs. foot), and could those same information-processing mechanisms be exploited to create needed anatomical structures in regenerative or even synthetic bioengineering settings?

As nature would have it, large-scale regeneration is not restricted to science fiction. Many invertebrates, such as hydra (Holstein et al. 2003), planaria (Elliott and Sánchez Alvarado 2013), and various arthropods (Maruzzo and Bortolin 2013), display perfect regeneration from injuries that would otherwise be fatal for many other organisms (Birnbaum and Alvarado 2008). Importantly, there are also several vertebrate models that serve as proof-of-principle for complex organ regeneration. For example, in salamanders, this capacity is retained well into adulthood (Brockes 1997), enabling regeneration of eyes, jaws, limbs, heart, ovaries, and spinal cord (Maden 2008; McCusker and Gardiner 2011). Other amphibians, such as frogs, retain the ability to regenerate up to a specific developmental stage (typically metamorphosis [Dent 1962]) but experience decline of regenerative capacity as they mature (Dent 1962).

Remarkably, instances of regeneration are also observed in non-amphibian vertebrates, from fish (Poss et al. 2003; Zupanc 2008; Sîrbulescu and Zupanc 2011) to mammals (Muneoka and Dawson 2020). Such instances of regeneration are typically restricted to specialized structures such as the lizard tail (Jacyniak et al. 2017; Lozito and Tuan 2017), mouse digit tip (Lehoczky 2017; Dawson et al. 2018; Seifert and Muneoka 2018), and deer antler (Kierdorf et al. 2007; Li et al. 2014), while wound healing in other tissues within these animals typically follows a general fibrotic response (Gurtner et al. 2008). Examples of regeneration exist even in humans; the human digit tip has been observed to regenerate in children (Illingworth 1974), although this regenerative capacity is di-

minished in adulthood (Shieh and Cheng 2015; Jafari et al. 2017). The routine, reliable, and very rapid growth of bone, vasculature, and innervation in adult deer antler (up to ~1 cm per day) suggests that there is nothing fundamental preventing complex appendages from regenerating in mammals (Price et al. 2005; Kierdorf et al. 2007; Li 2012).

Harnessing the power of the body's healing processes to stimulate the creation of a complex anatomical structure is a fundamentally daunting scientific prospect with tantalizing potential for addressing biomedical needs from birth defects to cancer to aging. Much work has been done over the last century to attempt to trigger this process in species that normally do not regenerate. While endogenous mechanisms in regeneration-competent species have been amply reviewed (Lehoczky 2017; Londono et al. 2018; Seifert and Muneoka 2018), the development of future biomedical therapies in this field depends on a thorough synthesis of prior results in nonregenerative models. Thus, here we provide an overview of what has been achieved by various interventions in five major categories: (1) surgical/engineered interventions, (2) biochemical pathway targeting, (3) murine transgenic lines with enhanced regenerative capacity, (4) targeted manipulations of cellular membrane potential, and (5) applied bioelectric interventions. We end with a perspective on promising future directions in this exciting, multidisciplinary field.

EPIMORPHIC REGENERATION: A BRIEF OVERVIEW

Naturally occurring vertebrate limb regeneration uses a regenerative process known as epimorphic regeneration to produce and pattern new tissues from the wound edge. Epimorphic regeneration begins with epithelial wound closure and the accumulation of a mass of undifferentiated cells; the resulting structure—the blastema (Allen et al. 2016; Seifert and Muneoka 2018; Muneoka and Dawson 2020)—is the source of new tissues. Rapid re-epithelialization of the wound bed and blastemal cell accumulation is followed by a thickening of the wound

epidermis, transforming it to a central blastemal signaling center known as the apical epithelial (or ectodermal) cap (AEC) (Han et al. 2005; Seifert and Muneoka 2018). The most highly regenerative vertebrates, salamanders, achieve this re-epithelialization in under 12 h postamputation (Repesh and Oberpriller 1978; Carlson et al. 1998), while other regenerative vertebrates, such as developing frogs, accomplish this in 24 h (Pearl et al. 2008; Beck et al. 2009). The regenerative AEC is crucial to proper epimorphic regeneration, as replacing the AEC with mature skin completely inhibits regeneration (Gidge and Rose 1944; Mescher 1976). In contrast, poorly regenerative vertebrates take 2 to 3 times longer to re-epithelialize, and fail to establish a functional AEC (Han et al. 2005; Londono et al. 2018; Muneoka and Dawson 2020).

It has been suggested that regeneration arises from a reactivation of the developmental mechanisms that drive limb outgrowth during development. One common family of genetic regulators implicated in vertebrate limb regeneration are fibroblast growth factor (FGF) proteins, having functional roles in limb outgrowth and morphogenesis with signaling functions in the apical ectodermal ridge (AER) of the developing limb bud (Martin 1998). In chick embryos, FGF8 and FGF10 have been shown to be endogenous inducers of limb bud formation (an apical ectodermal factor; Mahmood et al. 1995; Ohuchi et al. 1997), while ectopic treatment with FGF1, FGF2, or FGF4 similarly induces the formation of supernumerary limbs during development (Cohn et al. 1995). Interestingly, during limb regeneration in developing frogs (i.e., limb amputation prior to metamorphosis), FGF8 is promptly reexpressed in the newly formed AEC (Christen and Slack 1997). Likewise, salamander limb development and regeneration both use the expression of FGF8 in the AER/AEC, while other FGF proteins are exclusive to either limb development (FGF4, FGF10) or regeneration (FGF1, FGF2) (flanks, Christensen et al. 2002; and blastemas of *Ambystoma*, Dungan et al. 2002; Sun et al. 2002; Giampaoli et al. 2003). Conserved signals between development and regeneration also include bone morphogenic proteins (BMPs)

(Pajni-Underwood et al. 2007; Yu et al. 2010, 2012; Makanae et al. 2014; Norrie et al. 2014; Vieira et al. 2019), Msh homeobox proteins (Msx) (Davidson et al. 1991; Kostakopoulou et al. 1996; Koshiba et al. 1998; Han et al. 2003; Johnson et al. 2020), homeobox proteins (Hox) (Gardiner et al. 1995; Kostakopoulou et al. 1996; Nelson et al. 1996), and Sonic hedgehog (Shh) (Riddle et al. 1993; Chiang et al. 2001; Yakushiji et al. 2009). However, it remains an open question as to whether the high-level mechanisms that drive self-limiting morphogenesis toward a specific anatomical outcome are the same as those functioning in regeneration. Many efforts over the last 100 years have targeted diverse aspects of the process, in attempts to induce a limb-repair cascade in species that normally do not activate it after injury.

SURGICAL AND ENGINEERED INTERVENTIONS TO PROMOTE VERTEBRATE LIMB REGENERATION

Researchers have used various surgical approaches to improve regeneration, including the transfer of regenerative blastemal tissue and implantation of extracellular matrix (ECM) protein-based grafts. Early blastemal transplantation studies in *Urodeles* suggested that blastemal tissue was quite plastic and could adopt new regenerative fate if grafted onto heterotopic amputation sites (Weiss 1927; Schaxel 1934). However, it was later realized that, at a certain regenerative stage, the *Urodele* blastema becomes functionally independent of the host environment and will reliably regenerate all of the appropriate donor structures irrespective of where it is placed (Trampusch 1966; Stocum and Dearlove 1972; Pescitelli and Stocum 1980; Pecorino et al. 1996a,b).

In mouse digit tips, the nail bed is a known regulator and driving force behind successfully regenerating digit tips (Takeo et al. 2013; Leung et al. 2014). Interestingly, if the digit is amputated at the intermediate phalange, P2 (which is nonregenerative), grafting of a segment of P3 nail/nail bed epithelium induces minor bone growth directed upward toward the implanted nail epithelium (Mohammad et al. 1999), sug-

D. Davidian and M. Levin

gesting this epithelium is coordinating new bone growth. In contrast, grafting of regenerative fibroblasts derived from P3 blastemas into a host P2 amputation wound bed fails to induce any regenerative effect (Wu et al. 2013). Alternatively, if P2 fibroblasts are grafted into an amputated blastema forming P3, they will actively contribute toward regeneration of the P3 segment and restore P3 connective tissues. These findings suggest that the primary driver of epimorphic regeneration is a wound microenvironment conducive for regeneration, and that grafting of regenerative tissues alone is insufficient to drive full-scale regeneration. Additionally, these studies demonstrate that properly established regenerative environments have the capacity to reprogram nonregenerative cells (Wu et al. 2013).

Regenerative fibroblasts appear to have the capacity to participate in regeneration even if derived from nonregenerative origin tissue. However, regenerative success may be driven partly by the tissue microenvironment in which they are inserted. This is supported by studies showing that growth medium, conditioned by regenerative stem cells (i.e., containing bioactive compounds secreted by highly regenerative cells such as those responsible for deer antler regeneration [Shabbir et al. 2015; Li et al. 2017; Rong et al. 2019]), can be used to accelerate wound healing and enhance overall regeneration in cutaneous injuries when administered as a cell-free media (Li et al. 2017; Menéndez-Menéndez et al. 2017; Rong et al. 2019). This finding, taken together with the results demonstrating the modular nature of fibroblasts, suggests that a pro-regenerative tissue microenvironment can have great influence over the activity of the native cells and failure to establish a proper microenvironment may significantly impact the regenerative capability of tissue.

Surgical manipulation of developing limbs can shed light on potential drivers for limb regeneration. For example, if the hand of a developing mouse or frog embryo is modified surgically to bring together dissimilar tissue along an axis (e.g., anterior adjacent to posterior tissue), the resultant hand develops supernumerary digits (Wanek et al. 1989; Yokoyama et al. 1998)—a

phenomenon that has been interpreted as an intercalation rule that triggers growth at regions of nonadjacent positional information (Bryant and Iten 1977; Mittenthal and Trevarrow 1984; Crawford and Stocum 1988; Beck et al. 1999). This resembles the induction of supernumerary limbs in adult axolotls through the grafting of contralateral epidermis containing dermal cells of contrary axis identity (Endo et al. 2004). Ectopic growth also occurs upon grafting mouse embryonic limb buds onto amputated neonatal limbs. Grafting of the embryonic limb bud to an amputated forelimb of a neonatal mouse promotes significant bone and cartilage regeneration with the resulting regenerate complexity related to the developmental stage of the grafted limb bud (Fig. 1; Masaki and Ide 2007). Interestingly, the resulting regenerate outcome was not dependent on the native structure of the grafted limb bud, as grafts using cell limb bud homogenates formed equally complex regenerate structures (Masaki and Ide 2007). This suggests that a key determinant of limb outgrowth and morphogenesis during regeneration is the complement of cells and tissues in the regenerate's microenvironment.

An important driver and promoter of the blastemal microenvironment is the AEC (Shimokawa et al. 2012). In nonregenerative systems, the wound bed of an amputated limb or digit does not form a blastema but rather is slowly re-epithelialized with mature non-AEC epithelia through the migration of keratinocytes, fibroblasts, and myofibroblast-driven wound contraction (Martin 1997; Han et al. 2005; Gonzalez et al. 2016). This action of wound closure with mature epithelia typifies general fibrosis and this inclination toward fibrosis may be acting against potential regeneration. For example, in highly regenerative salamanders, covering of the wound with mature skin is known to inhibit regeneration (Mescher 1976). Interestingly, regenerative responses have been reported in nonregenerative vertebrates following the enforced inhibition of normal wound response re-epithelialization. For example, the formation of blastemal-like tissue was observed in P2 digit amputations using the super healing mouse strain, MRL-mice (Gourevitch et al. 2009),

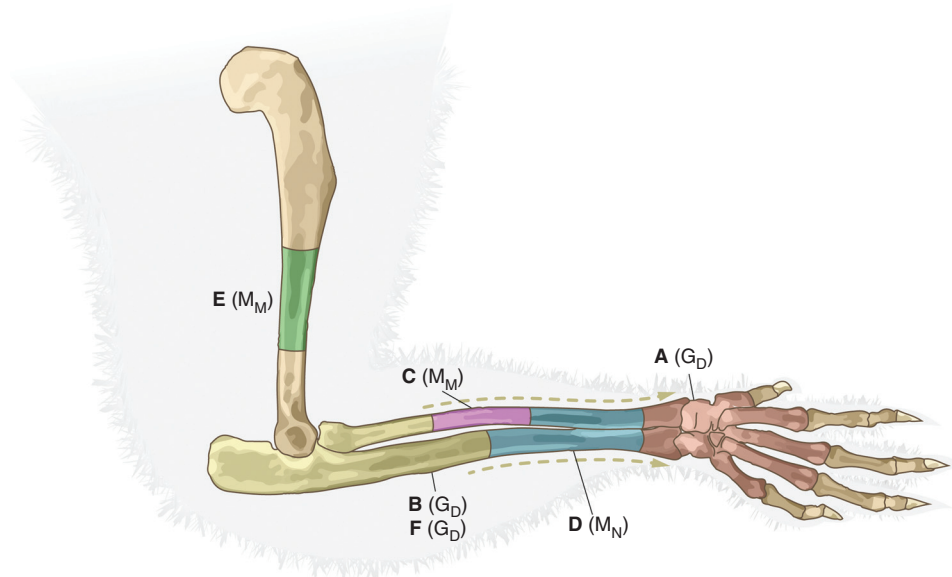


Figure 1. A schematic representation of bone growth in the context of experiments using targeted biochemical pathway treatments in mouse and rooster model(s). Colors are used to distinguish specific publications from one another and represent their reported growth. Data from Yu et al. (2012) (green) represents a medial amputation to the tibial bone transecting the fibula; this was concatenated to a forelimb representation over a humerus to conserve space. It is important to note that, anatomically, the tibia is proximal of the hind paw and distal to the femur. Colored dotted lines represent the entire growth area for a specific citation; these are only shown if other citation(s) overlap. (A) Based on Taylor et al. (1994), (B) based on Kostakopoulou et al. (1996), (C) based on Suckow et al. (1999), (D) based on Masaki and Ide (2007), (E) based on Yu et al. (2012), and (F) based on Makanae and Satoh (2018). (G_D) Developing *Gallus gallus* model, (M_N) neonatal murine model, (M_M) mature murine model.

which reportedly re-epithelialize the amputation at a rate 72 h slower than typical C57bl/6 strain mice (Turner et al. 2010a). This blastema-like tissue experienced waves of significant cell proliferation, but it also underwent waves of significant apoptosis that ultimately led to its destruction followed by standard wound closure and fibrotic healing (Gourevitch et al. 2009; Turner et al. 2010a). In similar fashion, blastema formation was reported in P2 digit amputations when the epithelial cell migratory blocker dibutyryl (db)-cAMP was administered to the wound bed (McCormack 1983). In addition, repeated mechanical removal of the wound epithelium along with repeated treatment with NaCl solution promoted blastema formation in P2 mouse digit amputations (Neufeld 1980). Limb regeneration was also induced in non-regenerative frogs through repeated epithelial

trauma to the amputated limb stump along with NaCl treatment (Poleżajew 1936; Rose 1945; Polezhayev 1946). These reports suggest that the mode by which nonregenerative systems cover the wound, using mature epithelium, is highly inhibitory to regeneration. This result may be attributed to the inability of mature skin to generate a proper regenerative microenvironment because it lacks the regenerative AECs. Indeed, the physiological properties of the overlying ectoderm (specifically, its ability to conduct ion flows across the epithelial barrier) have been suggested to be a driver for both the determination of the embryonic limb field and for regenerative capacity (Borgens 1984).

In addition to the importance of the wound covering, the deposition of underlying connective tissue is starkly different in regenerative versus nonregenerative wound healing. Fibrotic

D. Davidian and M. Levin

(scar forming) wound healing is characterized by significant deposition by tissue fibroblasts of connective tissue ECM, such as collagen I, in place of normal parenchymal tissue (Gurtner et al. 2008). Researchers studying wound healing in lower back cutaneous injuries of fetal mice discovered a lineage-restricted group of fibroblast cells, known as engrailed-1-lineage (En1) fibroblasts, responsible for the transition from scarless healing to scar-forming fibrosis (Jiang et al. 2018). Specifically, fibroblasts that expressed En1 during an embryonic state (EPFs, for En1-past expression fibroblasts) were shown to directly contribute toward fibrosis while En1-naïve fibroblasts (ENFs) do not (Rinkevich et al. 2015). Further analysis showed that grafting of EPFs in lower back wound beds promoted heavy deposition of collagen I and fibrosis while grafting of ENFs in the same injuries promoted scarless wound healing, a moderate and porous reticular ECM lattice (contrary to what is seen in dense cross-hatch fibrotic lattice), and increased blood vessel infiltration of the regenerate tissues (Jiang et al. 2018). Interestingly, an ENF-generated ECM lattice alone was sufficient to drive tissue wound healing toward a scarless fate (Jiang et al. 2018), showing that the underlying ECM is a significant regulator of regenerative outcome. The porous nature of the resulting ECM lattice deposited by these ENF cells is reminiscent of blastemal tissue, which is known to highly express matrix metalloproteinases (Santosh et al. 2011; Yates et al. 2012; Johnson et al. 2020) that degrade ECM components. Likewise, increasing collagen enrichment in the blastema directly inhibits regeneration in salamanders (Satoh et al. 2012).

The regenerative AEC and ECM dually promote regenerative healing, creating the appropriate microenvironment to stimulate epimorphic regeneration. In addition to AEC and ECM grafting, scaffolding materials typically composed of naturally occurring ECM components, or other organic compounds such as silk, can be manufactured and implanted into injured tissue fissures and act as a framework for the regenerate structure (Sundelacruz and Kaplan 2009; Benders et al. 2013; Caudwell et al. 2015). These scaffolds can be loaded with regen-

erative stem cells, bioactive compounds, or drugs to promote regeneration (Pritchard and Kaplan 2011; Yucel et al. 2014; Golding et al. 2016). In contrast to a regenerating limb, grafting treatments typically aim for targeted regeneration and restoration of specific tissues within a given organ structure, such as a fractured radial bone (Suckow et al. 1999) or a damaged heart valve (D'Onofrio et al. 2011). These engineered scaffolds, whether derived from synthetic or biological material, act as a foundation for natural growth of resident cells and tissues in which the scaffold is implanted. Several scaffolding techniques may have significant implications in the context of limb regeneration. Significant bone regeneration of a rat radial bone, which had been resected 11 mm at its center, was reported after grafting with decellularized porcine small intestinal submucosa (pSIS) scaffolds (Suckow et al. 1999). Specifically, rats provided with pSIS grafts showed about an 80% restitution of resected bone at 6 mo postsurgery with evidence of bone marrow formation (Fig. 1; Suckow et al. 1999). This same pSIS scaffolding technique was used to reconstitute canine Achilles musculotendinous junction following excision of the distal third of gastrocnemius muscle and proximal half of the associated Achilles tendon bundle (Turner et al. 2010b). After 6 mo, canines with pSIS scaffolds showed complete tissue regeneration, restoration of contractile force to ~50%, significant reinnervation with new neuromuscular junctions and significant muscular vascularization (Turner et al. 2010b). Similar success was observed in the restoration of skeletal muscle in mice using fibrin scaffolds (Page et al. 2011) or pSIS scaffolds (Valentin et al. 2010). More recently, decellularized human nail bed (dcNB) was used to construct an engineered scaffold (eNB) that differed from the dcNB, as it contained seeded bone mesenchymal stem cells (BMSCs) (Yu et al. 2019b). eNB scaffolds, when implanted into the back of nude mice, promoted the restoration of the nail plate and nail epithelium. Furthermore, expression of *Msx1*, an important component of regeneration and limb outgrowth (Kostakopoulou et al. 1996; Han et al. 2003; Johnson et al. 2020), was shown to be significantly expressed in eNB implants

compared to dcNB alone, BMSC alone, or sham control (Yu et al. 2019b). These engineering-based interventions show significant promise for regenerative interventions in vertebrates (for a more comprehensive review of scaffolding approaches, see Chen 2014 and Darnell et al. 2017).

These surgical and engineering-based interventions reveal key lessons about regenerative tissues and how they can be used to augment limb wound healing. A blastema, if provided time to reach a “critical mass,” can autonomously build its preordained missing tissues without needing positional information from its surroundings. However, blastemal cells are insufficient to alone drive regeneration if grafted into a nonregenerative environment. In addition to blastemal tissue, developing limb bud tissue, when grafted to amputated limbs of the same identity, can enhance regeneration but ultimately falls short of producing anything resembling the lost limb. Grafting of biologic composite material such as ECM scaffolds can indeed stimulate a regenerative response; in its current state, scaffolding approaches can be used to effectively modulate the regrowth of a specific tissue. However, in the case of limbs or digits, the complexity of the multitissue system has yet to be met with a sufficiently complex engineering solution. A perfusion decellularization approach was recently applied to an entire human cadaver forearm, preserving all ECM complexity and structure (Gerli et al. 2018). This decellularized matrix was posited to supply cells with perfectly organized, natural ECM to infiltrate as a means to regenerate the missing limb. However, cell-seeding technologies and challenges with nutrient supply deep within the developing tissue must be solved to successfully use this decellularized limb matrix.

BIOCHEMICAL PATHWAY TARGET INTERVENTION FOR INDUCING VERTEBRATE REGENERATION

Researchers have had success with techniques using limb developmental bioactive molecules to initiate a regenerative response in poorly or nonregenerative tissues. One family of signaling

molecules showing success in various nonregenerative models is the FGF proteins. FGF proteins are expressed in the apical epidermis in developing limb buds and are known to reexpress in these same regions following limb amputation in regenerative vertebrates (Christen and Slack 1997; Han et al. 2001, 2005; Giampaoli et al. 2003). In nonregenerative systems, this reexpression of FGF proteins is absent (Han et al. 2005). In addition, inhibition of FGF signaling within regenerative systems effectively blocks the formation of blastema and subsequent regeneration (Poss et al. 2000; Lin and Slack 2008). FGF proteins are such potent stimulators of limb growth that forced expression can rescue limb development following AER removal (Niswander et al. 1993; Fallon et al. 1994; Mahmood et al. 1995), or can even lead to the formation of ectopic limbs during development (Crossley et al. 1996; Ohuchi et al. 1997, an apical ectodermal factor). The importance of FGF signaling is underscored by regenerative neuronal dependence.

Early studies denervating regenerating Urodele limb stumps inhibited subsequent limb regeneration while grafting neuronal tissue to denervated limb stumps could rescue regeneration (Singer 1952; Thornton 1970). These experiments established the basis for neural dependence in Urodele regeneration that has been confirmed in other amphibious vertebrate regenerators (Simpson 1961; Endo et al. 2004; Mondia et al. 2011; Mitogawa et al. 2018). It was postulated that neurons are responsible for supplying the regenerating tissues with pro-regenerative bioactive molecules through neuronal secretion. This hypothesis is further supported by evidence showing that blastemal expression of FGF proteins is directly linked to innervation of the regenerating limb stump (Christensen et al. 2001; Satoh et al. 2017). Neurons in *Ambystoma mexicanum* (axolotl) synthesize FGF8 and BMP7 and transport these bioactive compounds to the regenerating limb stump through the axon (Satoh et al. 2016). In newts, nerve-dependent regeneration has been linked back to FGF2 expression in the AEC and inhibition of limb regeneration by denervation can be rescued by ectopic application of FGF2 at

D. Davidian and M. Levin

the limb amputation site (Mullen et al. 1996). Remarkably, ectopic limb growth can be stimulated in axolotl simply by deviating the innervating limb axon to an alternative location containing an epidermal lesion (Endo et al. 2004). Nerve dependency of ectopic limb formation in axolotl can be mimicked by implantation of beads soaked in BMP2, -7/FGF8, -2 in the proximal limb (Han et al. 2005; Makanae et al. 2014; Satoh et al. 2018; Vieira et al. 2019).

The regenerative potential of these neuronally associated bioactive molecules translates to other vertebrate systems as well. Ectopic application of FGF2 or FGF4 to amputated wing buds in developing embryonic *Gallus gallus* (red junglefowl) induced a robust regenerative response that often resulted in the complete reconstitution of the amputated limb (Taylor et al. 1994; Kostakopoulou et al. 1996). Specifically, treating developing limbs with FGF2 following distal zeugopod amputations resulted in the regeneration of missing zeugopod structures as well as the formation of some carpal and digit structures (Taylor et al. 1994). Similarly, amputated developing limb bud outgrowths of chickens, treated with FGF4, were able to develop complete humeral and zeugopod structures, and in some cases, incomplete autopod structures (Fig. 1; Kostakopoulou et al. 1996). Furthermore, in developing frogs and chickens, ectopic application of FGF2 and FGF8 on developing limbs with resected lower limb parts (presumptive zeugopods) resulted in the regeneration of the zeugopod (Fig. 1; Makanae and Satoh 2018; Satoh et al. 2018).

Innervation of a regenerating stump in Urodele is directly linked to the secretion of an additional neurotrophic factor, newt anterior gradient protein (nAG). nAG was found to be initially expressed in the neuronal sheath and subsequently in glands within the AEC (Kumar et al. 2007). Forced AEC expression of nAG was sufficient to rescue denervated limb buds leading to complete regeneration of aneurogenic limbs (Kumar et al. 2007).

Denervation of developing *Ambystoma maculatum* (spotted salamander) limb buds results in the formation of complete aneurogenic limbs (Popiela 1976) that, surprisingly, retain

full regenerative capacity (Yntema 1959; Steen and Thornton 1963). Kumar found that these aneurogenic limbs are capable of expressing the *A. maculatum* homolog to nAG (mAG) in their limb stump AEC despite being aneurogenic (Kumar et al. 2011), and reestablishment of neuronal dependence in these limbs inhibits the expression of mAG upon subsequent neural denervation (Kumar et al. 2011). This group also identified nAG homologs in mice, rats, frogs, and humans, which have yet to be characterized in the context of regeneration (Kumar et al. 2011).

In mature *Xenopus laevis*, increasing the neuronal innervation in a regenerating limb stump (hyperinnervation) drastically improves the resulting morphology of a limb regenerate, shifting regenerate outcome from a typically produced hypomorphic spike to an elongated regenerate with underlying structures more closely resembling a mature limb (Fig. 2; Mitogawa et al. 2018). Limb stump hyperinnervation increases blastemal expression of important growth and patterning genes: FGF2/-8, BMP7, *hoxa11/-13*, and *Shh* (Mitogawa et al. 2018). In the absence of hyperinnervation, forced blastemal expression of BMP7, FGF2/-8, and *Shh* via DNA electroporation leads to improved regenerate outcomes: increased length, enhanced cartilage structures and joint-like structures, similar to what is seen in hyperinnervated limbs (Mitogawa et al. 2018). Furthermore, induced expression of *Shh* in nonregenerative froglet limb amputations results in increased regenerative length and more complex patterning of regenerate bone (Yakushiji et al. 2009), similar to yet more moderate than what is seen with combinatorial approach of BMP7, FGF2/8, and *Shh* treatment. It should be noted that innervated stumps regenerated better overall, with more complex morphology, than those with supplemental gene expression alone (Mitogawa et al. 2018).

Likewise, the neurosteroid progesterone, which has been established as a potent promoter of wound healing and regeneration of both neural (Koenig et al. 2000; Chávez-Delgado et al. 2003; Rosales-Cortes et al. 2003) and nonneural injuries (McEwen 1991; Routley and Ashcroft 2009; including bone remodeling, Hennighausen and Robinson 2001), was shown to dramat-

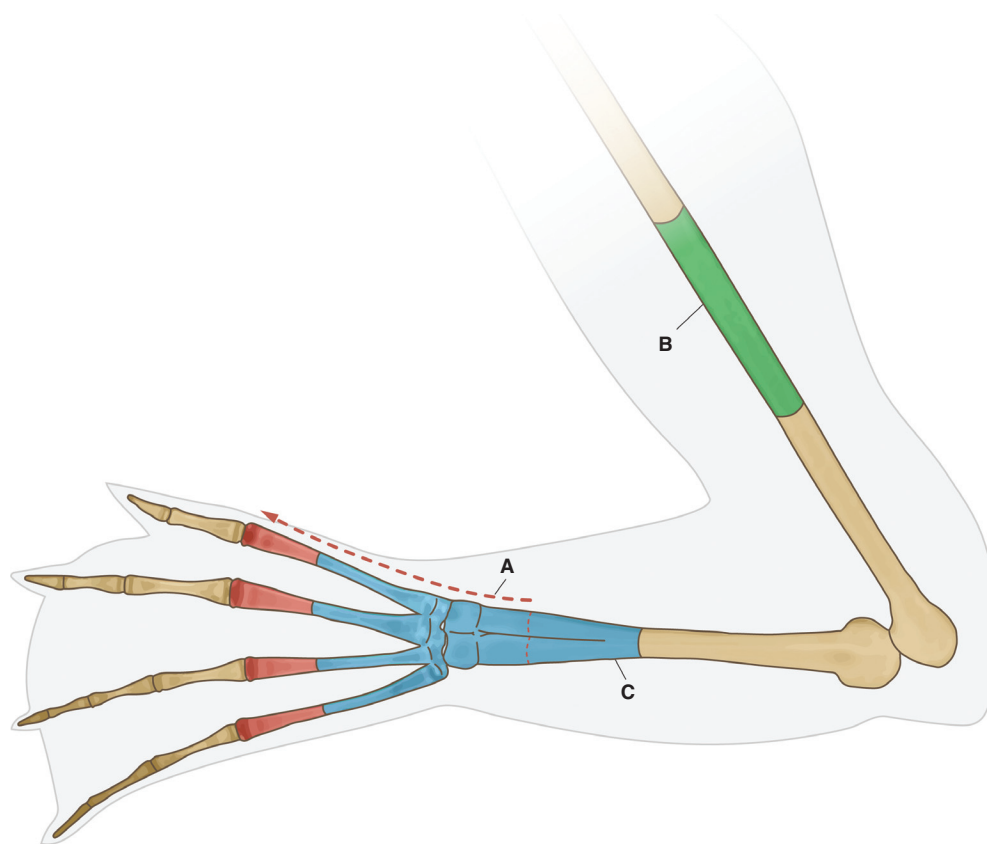


Figure 2. A schematic representation of bone growth in the context of experiments using targeted biochemical pathway treatments in mature Anura. Colors are used to distinguish specific publications from one another and represent their reported growth. It is important to note that Herrera-Rincon et al. (2018) amputations were performed at the midfemur of the hindlimb and are depicted here in the humerus to conserve space. Colored dotted lines represent the entire growth area for a specific citation; only shown if other shown citation(s) overlap. (A) Based on Lin et al. (2013), (B) based on Herrera-Rincon et al. (2018), and (C) based on Mitogawa et al. (2018). All studies used adult *Xenopus laevis*.

ically improve the regenerate outcome of adult *X. laevis* hindlimb amputees (Herrera-Rincon et al. 2018). Brief 24 h application of progesterone, delivered through a wearable silk-based hydrogel biodome device (Golding et al. 2016), resulted in a dramatic regenerative response lasting nearly 10 mo (Herrera-Rincon et al. 2018). Moreover, these partially regenerated hindlimbs developed a paddle-like morphology with highly vascularized and innervated tissues as well as significant femoral bone growth into the paddle structure (Fig. 2; Herrera-Rincon et al. 2018). Similarly, fibrin-based scaffolds seeded with

Shh + FGF10 + thymosin β 4 (T β 4) induced the near complete regeneration of forelimb wrist-level amputees in adult *X. laevis* (Lin et al. 2013). The regenerate hand contained intermediate skeletal elements with metacarpal bone, phalange epiphysial plates, and joint structures along with protruding digits (Fig. 2). This significant improvement in regeneration was underscored by the expression of known regenerative (and developmental) regulators Shh, Wnt3a, Wnt5a, FGF8, FGF10, and FGF20 (Lin et al. 2013). These outcomes, although significant improvements over hypomorphic spikes of

D. Davidian and M. Levin

controls, were not cosmetically similar to a normal forelimb, suggesting that important triggers of the limb regeneration cascade remain to be discovered.

Nonamphibious regenerative vertebrate models display contrasting dependence on nerve supply and regeneration. Early work in lizards shows that augmenting nerve supply, while not leading to the complete regeneration of a limb, can induce a moderate regenerative response (Simpson 1961; Singer 1961). In the murine digit regeneration model, there is strong evidence showing that neural tissue is involved in pro-regenerative paracrine signaling and denervation via sciatic nerve resection of the limb significantly reduces the ability of the digit tip to mount subsequent regenerative responses (Johnston et al. 2016). Furthermore, transplantation of Schwann cell precursor cells (SCPs), or local deposition of SCP paracrine factors platelet-derived growth factor AA or oncostatin M, can rescue digit denervation (Johnston et al. 2016). In contrast, a normally regenerated murine digit tip is significantly less innervated than its nonamputated counterpart, having 7.5-fold fewer axons in the connective tissue branches and 5.6-fold fewer in the bone marrow branch; but despite being significantly less innervated, this digit can fully regenerate with successive amputation (Dolan et al. 2019). This suggests neural dependence may be less of a driver for regeneration of these tissues than originally thought (Dolan et al. 2019). Can the regenerative capability of the digit tip be linked back to quantitative amounts of neural tissue, as it has been in amphibians (Singer 1952, 1954; Thornton 1970), and could mice continually mount a regenerative response in the digit tip with persistent amputations? This has yet to be tried in mice but evidence in axolotls suggests that even highly regenerative systems have their limitations when faced with repetitive assault (Bryant et al. 2017a,b).

While no treatments have led to complete regenerative rescue in proximal digit amputations to date, there are several targeted biochemical treatments that have shown promise in initiating a partial regenerative response. Mouse digit tips exposed to various develop-

mental growth factors demonstrate significant increases in regenerative capacity. For example, if FGF2 expression is induced through β -catenin stabilization, proximal P3 mouse digit tip amputations exhibit partial regeneration leading to an increased nail bed regenerate (Fig. 3; Takeo et al. 2013). Combinatorial treatment pairing mouse-induced pluripotent stem cells (iPSCs) with beads loaded with a cocktail of bioactive compounds, BMP2/FGF8/T β 4/Wnt3a on amputated mid-P2 digits, leads to significant regeneration of the lost P2 bone (Chen et al. 2017). This regenerative response is characterized by significant bone growth, increased length, and the formation of bone marrow structures in the newly formed bone (Fig. 3; Chen et al. 2017). Singular treatment with BMP2 in mouse digit P2 amputations leads to significant net bone outgrowth of over 60% (compared to sham control) in only 30 d posttreatment; with some mice even developing epiphyseal plate-like distal structures at 160 d postamputation (Fig. 3; Yu et al. 2012; Dawson et al. 2017). Interestingly, this response requires the periosteum layer of the bone (Dawson et al. 2017) and its removal abolishes the regenerative effects of BMP2 treatment (Dawson et al. 2017). This data links the known chondrogenic response of injured periosteal tissue (Colnot 2009; Dawson et al. 2016) as a proponent to this BMP2-mediated bone regeneration. Building upon these findings, researchers performed sequential treatment using BMP2 and BMP9 in mice following P2 digit amputation, where BMP2 was administered first to drive digit bone outgrowth, while subsequent treatment with BMP9 successfully stimulated the formation of a joint and epiphyseal plate (Yu et al. 2019a). The effectiveness of BMP2-mediated bone regeneration is not restricted to the digit, as midshaft hindlimb amputations treated with BMP2 also exhibit significant bone growth (Yu et al. 2012). Remarkably, BMP2-induced bone regeneration in these midshaft limb amputees successfully fused their tibia and fibula bones 8 wk postamputation in a morphologically accurate way (Fig. 1; Yu et al. 2012). Similarly, neonatal mice with mid-radial-ulnar forelimb amputations experienced significant bone re-

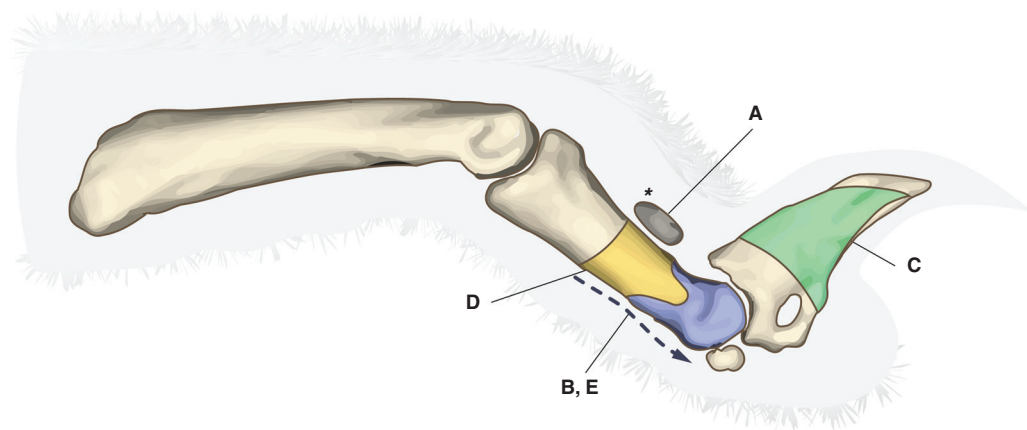


Figure 3. A schematic representation of bone growth in the context of experiments using targeted biochemical pathway treatments in mouse digit models. Colors are used to distinguish specific publications from one another and represent their reported growth. Colored dotted lines represent the entire growth area for a specific citation; only shown if other shown citation(s) overlap. Asterisk indicates formation of adjacent endochondral ossification centers lacking proper positioning with relation to cut boundary. (A) Based on Agrawal et al. (2011), (B) based on Yu et al. (2012), (C) based on Takeo et al. (2013), (D) based on Chen et al. (2017), and (E) based on Dawson et al. (2017). All studies used adult mice.

generation when gelatin beads containing BMP7 were implanted at the amputation site (Fig. 1; Masaki and Ide 2007).

A quite different approach was taken by one group of researchers who noted the importance of ECM breakdown during successful regenerative events. During regeneration-induced ECM breakdown, a small cryptic peptide is released into the local tissue (Agrawal et al. 2011). After isolating this cryptic peptide, they found that treatment of mid-P2 phalange amputations with this cryptic peptide-induced small ossification centers just adjacent to the amputation site (Fig. 3). Although this peptide could induce the formation of new bone (Agrawal et al. 2011), the new bone formation did not follow proper morphogenesis, suggesting that simply providing the cell-type building blocks of complex organs is not sufficient—patterning must be regulated or induced.

MURINE TRANSGENIC LINES WITH ENHANCED REGENERATIVE CAPACITY FOLLOWING DIGIT AMPUTATION

Establishment of transgenic inbred lines is commonplace in model-based research. With new

transgenic lines developed rapidly for various applications, some become well known for their proficiency to perform other tasks outside of their canonical purpose. In this section, we will discuss the remarkable discovery of enhanced regeneration found in two murine transgenic lines originally purposed for the study of non-wound healing systems.

In the early 1990s, researchers selectively bred murine B6, C3H, AKR, and large strains to develop the Murphy Roths large/lymphoproliferative (lpr) mouse strain (MRL/MpJ) (Watson et al. 1992). The capacity of these mice to perform scarless wound healing in multiple tissues, including dermal lesions (Beare et al. 2006; Davis et al. 2007; Buckley et al. 2011) and ear hole punch injuries (Clark et al. 1998; Fitzgerald et al. 2008), led them to be named “super super-healing” MRL mouse strain (Heydemann 2012). Classical regeneration observed in MRL mice is characterized by rapid wound re-epithelialization and formation of a proper regenerative blastema (Clark et al. 1998). When MRL mice were tested for their ability to mount a regenerative response following standard P3 digit amputation, it was found that MRL mice regrew their digits at an accel-

D. Davidian and M. Levin

erated rate compared to outbreed strains C57BL/6 and DBA/2 (Chadwick et al. 2007). In addition to accelerated re-epithelialization, a number of transcriptional differences were observed differentially expressed in regenerating P3 MRL mice, including a number of transcripts involved in Wnt signaling (LRP6) (Tamai et al. 2000), limb bud polarization factor (Formin-1) (Zeller et al. 1999), and growth factor regulators (SPARC) (Chadwick et al. 2007). When MRL mice were tested for more severe digit regeneration (amputations midway through the P2 phalange), they showed a unique propensity to form blastema-like tissues despite being unable to mount a formal regenerative response (Gourevitch et al. 2009). Still, MRL mice re-epithelialized their injuries more rapidly than the C57BL/6 or Swiss Webster strains against which they were tested. These reports of the wound re-epithelialization speed of MRL mice during P2 digit amputation are contrasted with other researchers' reports of significantly delayed wound re-epithelialization of MRL mice compared with C57BL/6 mice following mid-P2 phalange amputations (Turner et al. 2010a). Ultimately, reports of digit amputations in MRL mice demonstrate that, despite initial steps toward digit regeneration, MRL mice cannot sustain the blastema; cells undergo apoptosis, the blastema collapses, and regeneration is aborted and replaced with standard fibrotic wound healing (Gourevitch et al. 2009; Turner et al. 2010a).

In addition to this rather serendipitous finding, overexpression of *Msx1* and *Msx2* in vertebrates has proven effective in inducing regeneration in vertebrates. *Msx* proteins are readily expressed during the formation of a blastema in *Urodele* (Koshiba et al. 1998), *Xenopus* (Endo et al. 2000), and *Murinae* (Reginelli et al. 1995; Han et al. 2003; Lehoczy et al. 2011; Johnson et al. 2020), and have been shown to be required for successful regeneration (Han et al. 2003). Using the nonregenerative refractory period of the *Xenopus* model, researchers induced expression of *Msx1* using heat shock protein 70 promoter and showed that, although full regeneration was not achieved, *Msx1* regenerates showed

improved characteristics such as increased blastema accumulation, increased blastema outgrowth, thickened AEC, and increased number of toes forming as a result of treatment (Barker and Beck 2009). Following this study, researchers used a combinatorial approach of overexpression of both *Msx1* and *Msx2* in proximal nonregenerating P3 digit amputations in mice with high efficacy (Taghiyar et al. 2017). Specifically, bone-derived mesenchymal stem cells were modified to overexpress *Msx1* and *Msx2* and subsequently embedded at the amputation site 4 d postamputation. This treatment led to complete regeneration of the distal P3 bone 6 wk postamputation (Taghiyar et al. 2017). Overexpression of *Msx1* and *Msx2* brings critical gene-derived patterning information to the wound site, as it was shown that treated mice demonstrated increased expression of known patterning genes *BMP4* and *FGF8* (Taghiyar et al. 2017). Besides inducing these patterning genes, *Msx1* and *Msx2* have well-known roles in tissue patterning during development and regeneration (Reginelli et al. 1995; Bensoussan-Trigano et al. 2011; Lehoczy et al. 2011; Vieux-Rochas et al. 2013; Johnson et al. 2020) that likely contribute to the reported result (Taghiyar et al. 2017). The efficacy of this approach in supplying the wound site with patterning information is thought to be the key behind its success.

The RNA-binding protein *Lin28* was eventually used to create another strain of mice with significantly improved healing responses, *iLin28a* transgenic mouse or "*iLin28a* Tg" (Shyh-Chang et al. 2013). *Lin28* was first discovered in *C. elegans* where it was shown to be a regulator of developmental transition from a larval state into adulthood by controlling cell progenitor fate and renewal (Ambros and Horvitz 1984; Moss et al. 1997). Two *Lin28* paralogs, *Lin28a* and *Lin28b* (Viswanathan et al. 2008), are highly expressed in embryonic stem cells (Rybak et al. 2008) but are progressively lost as fetal development progresses toward adulthood (Shyh-Chang and Daley 2013). At the tissue level, *Lin28* is highly expressed in the embryonic epidermis and developing limb buds and is undetectable after birth (Yang and Moss 2003).

Because embryonic tissues are known to be highly regenerative compared to their adult counterparts (Deuchar 1976; Young et al. 1983; Alvarado and Tsonis 2006), researchers sought to use the delaying powers of Lin28 to force adult tissues into an embryonic-like state by overexpression of Lin28 in mice (Shyh-Chang and Daley 2013). The iLin28a Tg mice exhibited regenerative responses to hair follicle removal, ear hole punch injuries, and even neonatal proximal digit amputation (including the complete recapitulation of lost second phalangeal bone and soft tissue) (Shyh-Chang et al. 2013). Researchers found that regenerating bone of iLin28a Tg mice highly expressed Lin28, while that of wild-type mice lacked Lin28 expression (Shyh-Chang et al. 2013). Yet Lin28 expression failed to provide any regenerative potential in adult digit amputees (Shyh-Chang et al. 2013). Lin28 is most known for its function as a repressor of microRNA let-7 (let-7), although researchers analyzing Lin28-induced regeneration clearly demonstrate that let-7 repression, although necessary, is not alone sufficient to account for the observed regenerative responses (Shyh-Chang et al. 2013). In addition to its role in regulating let-7, Lin28 is a known regulator of translation for the metabolic enzymes Pfkfb, Pdha1, Idh3b, Sdha, Ndufb3, and Ndufb8, which have been shown through metabolic profiling to enhance oxidative metabolism (Shyh-Chang et al. 2013). The authors tested the contribution of Lin28 and its enhancement of oxidative metabolism by testing pharmacological compounds (3BP or 2-deoxy-D-glucose) targeting oxidative phosphorylation and their propensity to influence tissue repair. Pharmacological treatment with these compounds led to significant increases in tissue repair comparable to Lin28 induction groups (Shyh-Chang et al. 2013). In addition to its role as a repressor for let-7, Lin28 acts as a potent stimulator of regeneration through the regulation of cellular metabolic processes that ultimately led to a cellular microenvironment simulating a more embryonic state, thus enhancing the regenerative capacity of tissues (Reddien 2013; Shyh-Chang et al. 2013).

TARGETED MANIPULATIONS OF CELL MEMBRANE POTENTIAL (V_{mem}) FOR REGENERATION

All cells, not just neurons, communicate via bioelectric signaling (Levin et al. 2017). A key aspect of bioelectric networks in tissues are the spatial patterns of standing cell membrane resting potentials, V_{mem} , which regulate downstream cell behaviors and morphogenesis at the organ level (Levin and Martyniuk 2018). Targeting V_{mem} for the purpose of influencing wound healing and regeneration has grown in popularity as researchers begin to unravel all the cellular processes in which V_{mem} , and more broadly bioelectric signaling, regulate (Zhao 2009; Tseng and Levin 2013; Zhao et al. 2020) complementing classical work focused on trans-epithelial electric fields (Borgens 1982, 1983).

Bioelectric signaling has been shown to influence (and in many cases control) cellular migration (Stump and Robinson 1983; Nishimura et al. 1996), proliferation (Vodovnik et al. 1992; Sundelacruz et al. 2009; Barghouth et al. 2015), differentiation (Zhao et al. 2015; Liu et al. 2017; Yan et al. 2017), and neuronal growth (Patel and Poo 1982; Stump and Robinson 1983; McCaig and Rajnicek 1991), all processes vital for proper tissue regeneration and wound healing. Furthermore, a natural consequence of tissue injury is the generation of an electric current, known as an injury current, surrounding the wound site. In organisms with elevated regenerated capacity, injury currents are tightly regulated and efficiently drive migratory galvanotactic cell types such as neurons and immune cells toward the wound (Becker 1967; Adams et al. 2007; Reid et al. 2009).

In the context of wound healing and regeneration, bioelectric responses occur when the ionic microenvironment changes in response to tissue injury. These changes are induced by the destruction of the endogenous transepithelial potential (TEP) generated by conjoined epithelial cells that line all tissues (Zhao 2009). Injury of TEP-producing epithelia generates a region of depolarization at the injury site, which, when coupled with adjacent active TEP-producing epithelia, creates an electric di-

D. Davidian and M. Levin

pole. This generates an endogenous electric current (injury current) that travels through the resistive tissue matrix, creating an electric field (Nuccitelli 2003; Zhao 2009). Endogenous currents, and the fields they generate, act directly on membranes of cells within the field, enabling them to orient to and migrate along electric field lines leading directly to the wound (Gross et al. 1986; McCaig et al. 2009; Kucerova et al. 2011; Yao et al. 2011; Cao et al. 2014). Manipulating these currents in injured tissues can precisely alter subsequent wound healing responses. For example, treating the wound bed of murine corneal injuries with aminophylline (an enhancer of chloride flux leading to an increased TEP within adjacent healthy epithelium) nearly doubles the rate of wound healing (Song 2004). In addition to accelerated wound healing, neuronal invasion and directedness in the corneal tissue was increased as a result (Song 2004). Manipulation of transepithelial electric fields is currently a very promising target for a number of tissue-level repair contexts (Zhao et al. 2006, 2020; Reid et al. 2011).

Tadpole tails, which contain a complex pattern of spinal cord, muscles, nerves, and vasculature, are regenerative from the moment of initial tail growth up until the tail is lost during development (Beck et al. 2009). However, there is an intermediate period during which the tail cannot regenerate; but after this refractory period (Beck et al. 2003; Ivanova et al. 2018), regenerative capacity is regained until metamorphosis (Beck et al. 2003). Amputated tadpole tails exhibit temporal changes in V_{mem} at the amputation site coincident with the state of their regenerative capability (Adams et al. 2007). In regenerating tails, V_{mem} at the amputation site undergoes an initial depolarization at 6 h post-amputation followed by a repolarization of the tissue 24 h postamputation (Adams et al. 2007). During the refractory period, the initial depolarized state at the amputation site persists and is indicative of an inability to mount a regenerative response (Adams et al. 2007). These underlying bioelectric signatures of regeneration in the tadpole tail are supported by measurements of currents in amputated tadpole tails. Proper tadpole tail regeneration was marked by an initial out-

ward current that later reversed to an inward current (known as a rectifying current) between 12 and 24 h postamputation (Reid et al. 2009). Later, it was discovered that O_2 flux, reactive oxygen species production, and hypoxia-inducible factor 1α (HIF- 1α), a master regulator of O_2 homeostasis, mediate tadpole tail regeneration (Ferreira et al. 2018). Interestingly, HIF- 1α stabilization can be used to promote tail regeneration during the refractory period and was shown to regulate endogenous electric current reversal occurring in normally regenerating tail buds (Ferreira et al. 2018). These temporal bioelectric dynamic changes within the tadpole tail are required for proper regeneration; this is supported by work showing that inducing these known shifts in bioelectric state during the refractory period can rescue regeneration (Adams et al. 2007; Reid et al. 2009).

During the tadpole tail regeneration, regenerative potential is eliminated through the inhibition of proton pump (H^+ V-ATPase) caused by the failure of tissue to repolarize within 24 h following amputation; this repolarization is required for up-regulation of *Msx1*, *Notch*, and other key regenerative genes (Adams et al. 2007; Tseng et al. 2010). The importance of this bioelectric state was further illustrated by research showing that the forced expression of a yeast H^+ pump (PMA1.2) during refractory period tail amputations rescued regeneration of refractory tails and tails in which endogenous V-ATPase activity was abrogated (Adams et al. 2007). Because frog H^+ V-ATPase has no sequence or structural homology to the PMA1.2 that can substitute for it, these data show that the necessary and sufficient signal for tail regeneration is not a specific gene product, but a physiological state.

Later, it was found that regenerating tadpole *X. laevis* tails activate H^+ V-ATPase activity 6 h postamputation, which leads to a downstream activation of Na^+ currents through voltage-gated sodium channels (Na_V). This local Na_V activation leads to downstream activation of a key transcriptional regulator, sodium-induced kinase, which acts to regulate the transcription of known regenerative modulators *Msx1* and *Notch*, thus leading to proper tail regeneration

(Tseng et al. 2010). Furthermore, to elicit more precise control over proton current, researchers showed that introduction of a light-gated Archaelhodopsin-based H^+ -ATPase rescued tail regeneration during normal tadpole tail refractory periods, while allowing for precise optogenetic channel activation via exposure to 463 nm light source (Adams et al. 2013). These studies clearly demonstrate the potential for bioelectric mechanisms to govern regeneration and demonstrate the ability to exploit these measures as tools to induce regeneration in otherwise non-regenerative tissues. Importantly, the sodium flux can be induced by an ionophore—a small molecule signal that does not require transgenes and is therefore more suitable for application in human patients (Tseng et al. 2010).

APPLIED BIOELECTRIC INTERVENTIONS STIMULATING VERTEBRATE REGENERATION

While molecular bioelectrics targets native ion channels or V_{mem} , a more classical approach uses electrodes to deliver external electric fields to modulate tissue bioelectric state. One example used a bimetallic electrode (a fusion of platinum and silver wire) with a measured electric field of 66.7 mV/mm in Ringers solution (Smith 1967). Implantation of this electrode at the bed of an amputated adult frog forelimb (*Rana pipiens*) led to a significant regenerative response resulting in several millimeters of growth, wound closure by a thickened epithelium, formation of a blastema-like structure, and regeneration of loose poorly differentiated mesenchymal tissue, all within a 3 mo period (Fig. 4; Smith 1967). Later experiments using the same nonregenerative adult *R. pipiens* forelimb model, with a slightly modified battery-powered implantation device, reinforced the potential for applied current to stimulate regeneration and revealed that anatomical positioning of electrodes had a significant impact on the regenerative potential of this treatment (Smith 1974). It was discovered that dorsal-postaxial placement of the anode, delivering 1.0×10^{-7} A over 1 mo, resulted in significant forelimb regeneration measured 4-mo postamputation. Moderate re-

generation (increased bone and tissue growth) was observed in 16 of 21 cases while remarkable regeneration (characterized by the formation of moveable digits) was shown in five of 21 cases. Most notably, one of these five animals regenerated a complete forelimb indistinguishable from the original, with all digits and internal structures properly formed and oriented (Fig. 4; Smith 1974). In the instance of full limb regeneration, researchers allowed this frog 1 yr to regenerate as the organism displayed a continued regenerative response (Fig. 5A–D; Smith 1974). Borgens later revisited these experiments in 1977 using the same model organism and electrode implant techniques, including electrode placement and dipole orientation. However, the magnitude of current applied in these experiments was approximately double to that used by Smith (0.2 μ A vs. 0.1 μ A). Likewise, Borgens et al. (1977) reported noteworthy regeneration in frogs treated with applied currents, observing the formation of new bone and bone-like cartilage structures, new muscle and nervous tissue, despite no formation of new digits or complete forelimbs (Fig. 4). These findings also corroborated the importance of electrode placement as well as dipole orientation underlying this regenerative response (Borgens et al. 1977).

Remarkably, electrode implants have also proven effective in murine limb regeneration. Becker assessed the potential for bimetallic electrode implantation to induce regeneration in Sprague–Dawley rats, whose forelimbs were amputated at the lower 2/3 of the distal humerus. Implantation of these devices resulted in blastema formation followed by significant bone and tissue regeneration (Becker 1972). In contrast to Smith's bimetallic electrode, Becker's electrode was modified by a 10 M Ω resistor to yield delivered currents ranging from 3 to 6 nA, which was reported to lead to the regeneration of the lost humeral bone, in some cases including the formation of a joint. In these experiments, 21 animals were used, with 10 analyzed at or before 7–11 d postamputation (Becker 1972). Much of the remarkable regeneration was seen in animals given between 12 and 28 d to regenerate. In this limited group of 11 animals, two formed an initial blastema that eventually was lost to fibrosis;

D. Davidian and M. Levin

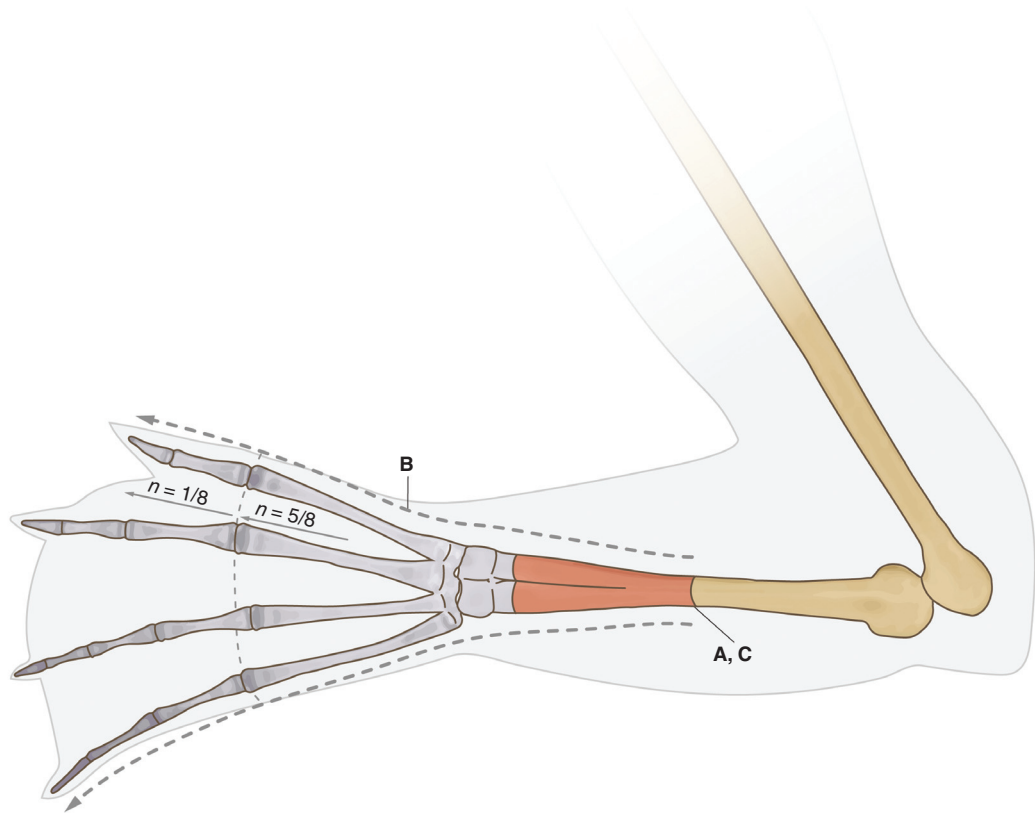


Figure 4. A schematic representation of bone growth in the context of experiments using applied electric currents in Anura. Colors are used to distinguish specific publications from one another and represent their reported growth. Colored dotted lines represent the entire growth area for a specific citation; only shown if other shown citation(s) overlap. (A) Based on Smith (1967), (B) based on Smith (1974), and (C) based on Borgens et al. (1977). All cited examples used a mature *Rana pipiens* model.

three showed significant blastemal response with bone, cartilage, and muscle regrowth; and six displayed even more impressive regeneration, having near complete distal humeral restitution with two epiphyseal centers. In one case (within the group of six), Becker observed the formation of a complete humeral epiphysial plate along with a complimentary joint (Fig. 6). Another surprising finding was one instance of the formation of a supernumerary humerus, preceded by a larger than normal blastema (Becker 1972). Unfortunately, the actual current of the devices used was not reported. Nevertheless, this influence of electric current on bone formation is complemented by prior work showing that endogenous electric currents arise

from naturally occurring formation of biological PN (positive and negative) junction diodes through collagen and apatite networks that translate mechanical forces to electrical currents (Becker 1967). As bone is introduced to load and compression forces, it will deposit new bone on the concave/compressed side in correspondence with the endogenously formed cathodal surface generated by these collagen/apatite junctions (Becker 1967).

These findings of electrically induced rat limb regeneration would be later corroborated by Smith in 1981. Smith performed mid-antebrachium amputations in Sprague–Dawley rats and implanted the same bimetallic electrode that he used in frog forelimb amputations in

Inducing Limb Regeneration

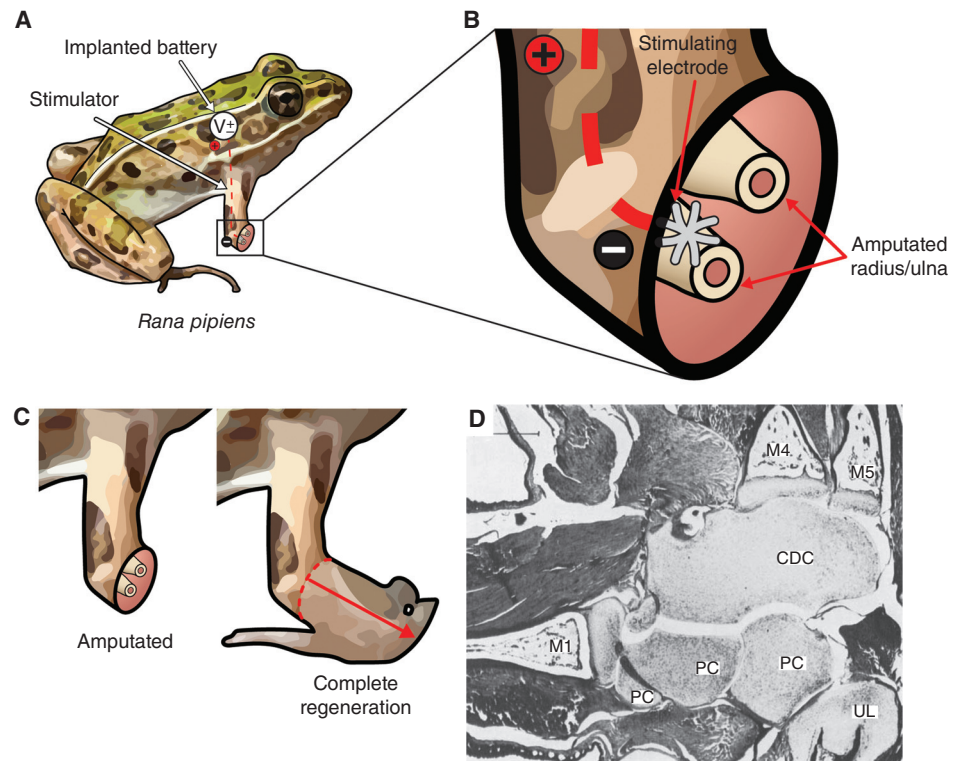


Figure 5. Summary schematic showing a specific example of regeneration induced by applied electric current in the adult frog, *Rana pipiens*. (A) Illustration of adult *R. pipiens* frog showing the amputation plane at the first 1/3 of the forearm and the placement of the embedded stimulating wire connected to a battery delivering 0.1 μ A of current to the wound site. (B) Enhanced illustration showing the wound site and placement of the negative stimulating electrode at the dorsal-postaxial region of the amputation plane. (C) Illustration showing the resultant regeneration of an individual frog, a complete regrowth of the lost tissue, which was reported as the best regenerate of the study (note that one digit grows at an angle, as is normal for this species). (D) Excerpt from Smith (1974) showing a cross section of the palm of the regenerated arm with labeled segments. (M1, M4, M5) Bases of metacarpals, (UL) ulnar, (PC) proximal carpal, (CDC) common distal carpal. (Panel D from Smith 1974; reprinted, with permission, from John Wiley and Sons © 1974.)

1974 (Smith 1974), with cathodal placement in the dorsal-postaxial region above the ulna at the amputation surface (Smith 1981). Similar to his work in frogs, Smith observed significant bone, skeletal muscle, and cartilage regeneration, and in some cases the early stages of joint formation (Fig. 6; Smith 1981). It should be noted that the polarity of the electric field induced by Smith's electrode placement, and magnitude of current (1 μ A; \sim 1000X greater than Becker's), within the forelimb is contrary to that done by Becker in humeral amputations. Nevertheless, Smith's observations confirm the ability of electric cur-

rents to stimulate significant regeneration in murine limbs. Despite these compelling reports, not much work has been done recently to decipher the significant regenerative capacities induced through bioelectric intervention, with most attention being paid to biochemical and genetic control mechanisms. This trend parallels the history of bioelectrics in developmental biology, although the development of modern molecular tools and the integration of bioelectric signaling with transcriptional cascades has begun to shed increasing attention on the importance of ion current- and voltage-based

D. Davidian and M. Levin

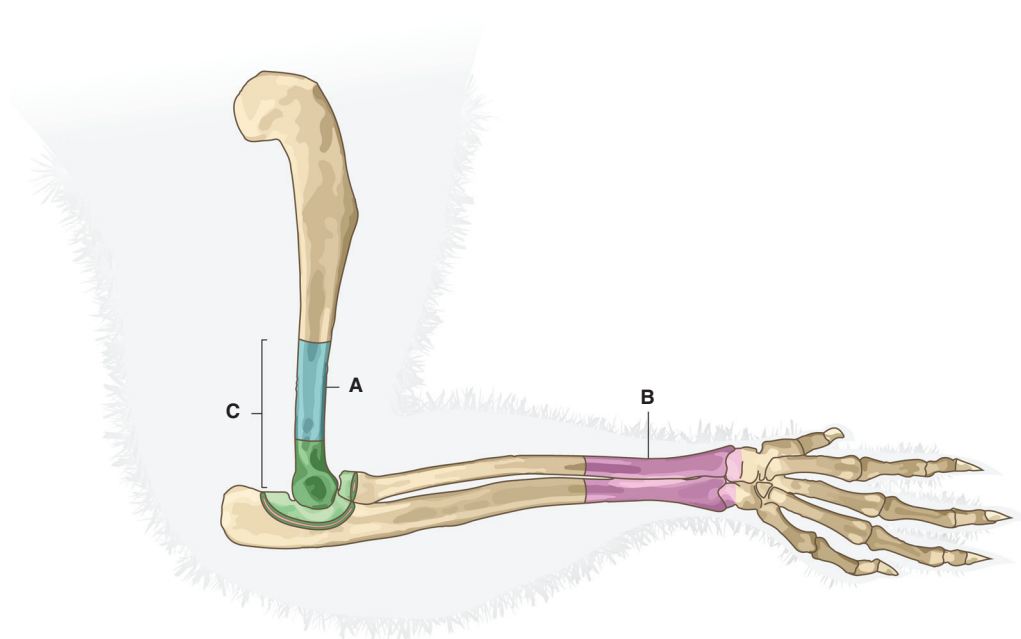


Figure 6. A schematic representation of bone growth in the context of experiments using applied electric currents in Muridae. Colors are used to distinguish specific publications from one another and represent their reported growth. (A) Based on work in Libbin et al. (1979), (B) based on work in Smith (1981), and (C) based on work in Leppik et al. (2016). Both examples were performed in the Sprague–Dawley rat model.

mechanisms (Nuccitelli et al. 1986; Bates 2015; Levin 2020, 2021).

Leppik et al. recently revitalized this approach (Becker 1972; Libbin et al. 1979), demonstrating the capacity for applied electric currents to stimulate regeneration in nonregenerating rat limbs. Using the bimetallic electrode implant, Leppik observed that, within a 28 d regeneration period, electrically stimulated rat limbs showed significant regeneration with substantial bone growth, increased vascularization of regenerate tissue, and decreased neuromas (Fig. 6; Leppik et al. 2016). Although both Leppik and Libbin described a reduced effect compared to that reported by Becker (Fig. 6), two significant electrically driven results are noteworthy. First, neuroma formation is characteristic of fibrotic healing postinjury (Watson et al. 2010), and electric stimulation completely inhibited neuroma formation (Leppik et al. 2016). Second, normal fibrotic healing of an amputated limb (or proximal digit) results in rapid capping of the bone marrow cavity (Turner et al.

2010a). Electrically stimulated limbs showed a prolonged opening of the marrow cavity that remained open for as long as 7 d postamputation compared to control animals whose marrow was completely capped by 7 d postamputation (Leppik et al. 2016). Bone marrow is known to be rich in mesenchymal stem cells that play a significant role during bone repair (Colnot 2009) and have been heavily investigated for their capacity to rejuvenate numerous tissue types (Penforis and Pochampally 2011). Thus, marrow access into the regenerating tissues may have contributed to the regeneration observed in electrically stimulated limbs.

In 2010, a group of researchers approached the use of electrical stimulation in a novel way by creating a bioreactor coined “BioDome” (Hechavarria et al. 2010). The BioDome is designed to maintain a hydrated environment at the wound interface while delivering bioactive compounds and electrical stimulation to the amputation site. The key component of this bioreactor is its implemented hydrogel. This hydrogel pro-

vides the hydrated environment, osmotic control over the wound, and acts as a precise delivery mechanism for embedded bioactive compounds whose release kinetics are regulated by the properties of the hydrogel, which can be carefully manipulated (Pritchard and Kaplan 2011). Integral to this design is the capability not only to deliver a drug or growth factor of choice to the wound, but also to simultaneously treat the wound with electrical stimulation to modulate its bioelectric state. Control over the wound's bioelectric state alone has been shown to have the capacity to induce regeneration in nonregenerative vertebrates (Jenkins et al. 1996; Tseng et al. 2010; Adams et al. 2013; Leppik et al. 2016). Coupling this with bioactive compound delivery may prove to be a highly effective therapeutic.

CONCLUSION: MECHANISMS CONTRIBUTING TO REPORTED REGENERATIVE IMPROVEMENT

Appendage regeneration is in a unique position to contribute therapies that significantly improve quality of life. Accelerating research in regenerative fields has already borne fruit with studies developing techniques to regenerate significant amounts of lost tissue (Suckow et al. 1999; Kumar et al. 2007; Yakushiji et al. 2009; Turner et al. 2010b; Yu et al. 2012; Lin et al. 2013; Herrera-Rincon et al. 2018) and even features such as joints that closely resemble healthy structures (Yu et al. 2019a). Five general approaches have been used to achieve varying degrees of regeneration in poorly regenerative vertebrate systems: surgical intervention, biochemical pathway targeted interventions, selective breeding, pharmacological V_{mem} augmentation, and exogenously applied electric fields. Targeted manipulation of biochemical pathways via systemic or local treatment with pharmacological substances has proven to be the most effective and reproducible means to induce vertebrate limb regeneration in nonregenerative systems. Taken together, the body of work on regenerative induction suggests a few common features (summarized in Table 1).

Targeting native biochemical pathways to induce regeneration is promising because it uses cells' native capacity to grow tissue, predi-

cated by embryonic development but perhaps suppressed through evolutionary time. These therapies are designed to rejuvenate cellular mechanisms that emulate those used during development and repurpose them for adult limb regeneration. Of the various biochemical stimulators discussed, those employing BMP and FGF proteins are the most effective and consistent stimulators of limb outgrowth across non-regenerative adult vertebrate systems (Taylor et al. 1994; Kostakopoulou et al. 1996; Mullen et al. 1996; Christen and Slack 1997; Yu et al. 2010, 2012, 2019a; Lin et al. 2013; Takeo et al. 2013; Vieira et al. 2019). Treatments with BMP2 (Yu et al. 2012, 2019a) and BMP9 (Yu et al. 2019a) in mice were highly effective at partial regeneration of amputated limbs as these treatments significantly enhanced underlying bone and joint regeneration. Bone outgrowth is a known determinant of successful regeneration in nonregenerative vertebrates (Sensate and Marques-Souza 2019). The effectiveness of BMP and FGF in stimulating limb regeneration can be seen from amphibious (Makanae et al. 2014; Satoh et al. 2016; Vieira et al. 2019) to mammalian vertebrates (Han et al. 2003; Yu et al. 2012, 2019a), and ongoing research may yet discover how BMP's may be used to successfully and completely regenerate lost limbs.

Interestingly, the only ever reported instance of inducing complete vertebrate appendage regeneration occurring in a nonregenerative system was achieved through the manipulation of bioelectrics (Smith 1974). This outcome has yet to be reproduced with modern tools and molecular characterization, but the recent successes of modulation of resting potential to manipulate human (Sundelacruz et al. 2008, 2013, 2016) and rodent (Feng et al. 2017; Mobini et al. 2017) stem cells and amphibian tail and limb regeneration (Fig. 7A–F; Adams et al. 2007, 2013; Tseng et al. 2010) suggest that bioelectric interventions are likely to be a key modality (Herrera-Rincon et al. 2017). Bioelectric controls of cell behaviors (Blackiston et al. 2009) and tissue-level morphogenetic processes (Reid et al. 2009; Lois et al. 2010; Perathoner et al. 2014; Bates 2015; Ferreira et al. 2016, 2018; Dahal et al. 2017; Daane et al. 2018; Lanni

D. Davidian and M. Levin

Table 1. Scored results from reported observations across the various bodies of work investigated in this review

References	Model	Age	Amputation	Treatment	Time	B/C	M	N
Smith et al. 1967	<i>Rana pipiens</i>	Adult	Radial/ulnar	0.67 V/cm (Ringers)	Until sac.	++	++	NR
Becker 1972	<i>Rattus</i>	Adult	Humeral	$3-5 \times 10^{-9}$ Å (Ringers)	Until sac.	+	+	NR
Smith et al. 1974	<i>R. pipiens</i>	Adult	Radial/ulnar	1.03×10^{-7} Å (tissue)	30 d	+++*	+++*	NR
Borgens et al. 1977	<i>R. pipiens</i>	Adult	Radial/ulnar	2.0×10^{-7} Å (tissue)	21–30 d	+	+	+
Libbin et al. 1979	<i>Rattus</i>	Adult	Humeral	$3-10 \times 10^{-9}$ Å (NR)	4–14 d	+	-	NR
Smith et al. 1981	<i>Mus musculus</i>	Adult	Radial/ulnar	1.04×10^{-6} Å (NR)	Until sac.	++	++	NR
Taylor et al. 1994	<i>Gallus gallus</i>	Embryonic	Radial/ulnar	FGF2	Until sac.	+++	NR	NR
Kostakopoulou et al. 1996	<i>G. gallus</i>	Embryonic	Radial/ulnar	FGF4	Until sac.	+++	NR	NR
Suckow et al. 1999	<i>M. musculus</i>	Adult	Radial	Porcine small intestinal mucosa	Until sac.	+++	NR	NR
Masaki and Ide 2007	<i>M. musculus</i>	Neonatal	Radial/ulnar	Gelatin + BMP7	Until sac.	++	NR	NR
Turner et al. 2010b	<i>Canis lupus familiaris</i>	Adult	Achilles	Porcine small intestinal mucosa	Until sac.	NR	+++	+++
musculotendinous junction								
Agrawal et al. 2011	<i>M. musculus</i>	Adult	P2 digit	Cryptic peptide	Until sac.	+	NR	NR
Yu et al. 2012	<i>M. musculus</i>	Adult	P2 digit	BMP2	Until sac.	+++	NR	NR
Yu et al. 2012	<i>M. musculus</i>	Adult	Tibia/fibula	BMP2	Until sac.	++	NR	NR
Lin et al. 2013	<i>Xenopus laevis</i>	Adult	Wrist	β-Catenin limb bud cells + (Shh, FGF10, Tβ4)	Until sac.	+++	+++	+++
Takeo et al. 2013	<i>M. musculus</i>	Adult	Proximal P3 digit	Stabilized β-catenin	Until sac.	+++	NR	NR
Leppik et al. 2016	<i>Rattus</i>	Adult	Humeral	Applied current (not measured)	Until sac.	+	-	-
Chen et al. 2017	<i>M. musculus</i>	Adult	P2 digit	iPSC + (BMP2, FGF8, Tβ4, WNT3a)	Until sac.	++	NR	NR
Dawson et al. 2017	<i>M. musculus</i>	Adult	P2 digit	BMP2	Until sac.	+++	NR	NR
Makanae and Satoh et al. 2018	<i>G. gallus</i>	Embryonic	Radial/ulnar	FGF2, FGF8	Until sac.	+++	NR	NR
Herrera-Rincon et al. 2018	<i>X. laevis</i>	Adult	Femur	Progesterone	24 h	++	+++	+++
Mitogawa et al. 2018	<i>X. laevis</i>	Adult	Radioulna	Hyperinnervation	Until sac.	+++	+++	NR
Mitogawa et al. 2018	<i>X. laevis</i>	Adult	Radioulna	BMP7, FGF2/-8, Shh	Until sac.	++	NR	NR

Regeneration was scored from + = little regeneration to ++++ = complete regeneration (+++* = significant regeneration with 1 instance of complete regeneration). Although no score of +++++ was given to any report, various works did exemplify high levels of regeneration (+++). When reporting values of applied current, parentheses are used to describe the medium in which the current was measured, as this holds significance in comparing across experimental reports. Time refers to the amount of time a given treatment was applied (not the amount of time the animals were given to regenerate). Until sac. = treatment was applied until animals were sacrificed.
(B/C) Bone and/or cartilage, (M) muscle, (N) nerve(s), (NR) not reported.

Inducing Limb Regeneration

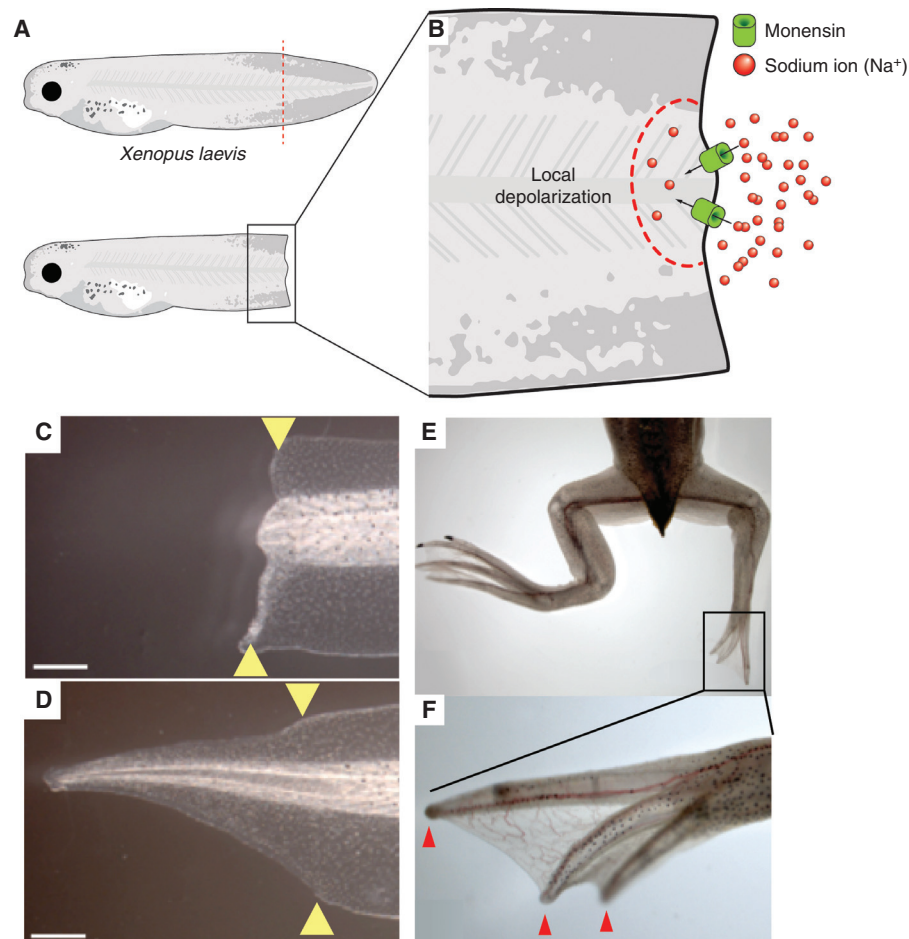


Figure 7. Summary schematic showing the effects of monensin treatment used to rescue regeneration in *Xenopus laevis* appendages. (A) Illustration of *X. laevis* tadpole at developmental stage ~45 during what is known as the refractory period (nonregenerative), showing intact and amputated specimens. (B) Enhanced illustration showing the mechanism by which monensin (a sodium ionophore) locally depolarizes the tail amputation site. (C) Morphology of a tail 8 d after being amputated during the tadpole refractory period, showing no growth. (D) Morphology of a regenerated tail that was also amputated during the refractory period and treated with a 1-h monensin soak, demonstrating its ability to rescue regeneration. (Panels C and D from Tseng et al. 2010, reprinted under a Creative Commons Attribution-Noncommercial-Share Alike 3.0 Unported License [CC-BY-NC-SA].) (E) *Xenopus* froglets, at the nonregenerative stage, exhibit regeneration of hindlimbs when treated for 24 h with a monensin soak (Tseng and Levin 2013). (F) Close-up of distal regenerate showing fairly normal resultant structure and morphology. Yellow arrowheads in panels C and D indicate amputation plane. Red arrowheads indicate new digits. Scale bars, 500 μ m. (Panels C and D used with permission from Tseng et al. 2010; panels E and F kindly provided by AiSun Tseng [Levin laboratory].)

et al. 2019; Levin 2021) can act during multiple steps thought to be part of the regenerative control cascade (Fig. 8). Overall, it is likely that successful outcomes will be achieved by approaches with two components: wearable bioreactors to provide a regeneration-permissive, supportive

environment, and a combination of bioelectric, biochemical, and haptic signals that trigger growth and initiate self-limiting, locale-appropriate morphogenetic cascades. By perfecting these aspects for limb regeneration, it is likely that the progress will lead not only to applied

D. Davidian and M. Levin

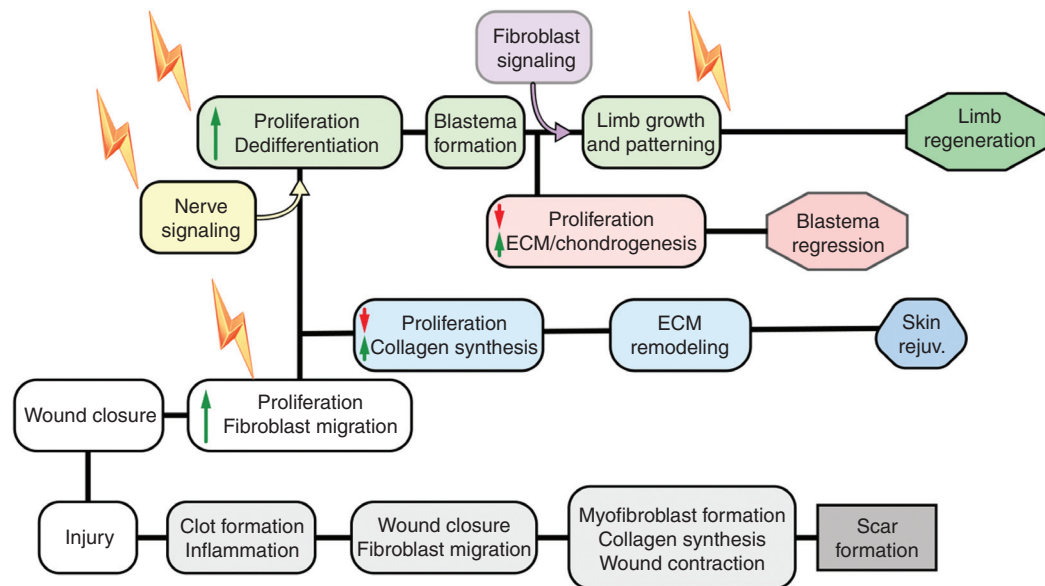


Figure 8. Flowchart summarizing the various processes and outcomes following injury in the context of wound healing and regeneration. This diagram was constructed after Figure 2 of Gardiner (2005) as a foundation; yellow lightning symbols indicate processes where bioelectric signaling can work as a regulatory trigger (including effects on cell proliferation, guidance of innervation, control of differentiation and immune cell migration, and tissue-level morphogenetic decisions). (ECM) Extracellular matrix. (Permission for modification of Figure 2 by Gardiner 2005 granted by Mary Ann Liebert © 2005.)

biomedical outcomes but also to a much deeper basic understanding of the endogenous controls of growth and form and the plasticity with which they can be controlled.

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D. Davidian and M. Levin



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Inducing Limb Regeneration



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D. Davidian and M. Levin

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D. Davidian and M. Levin

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