Dynamical Decoupling of Nitrogen-Vacancy Electron Spins in Diamond and Nanodiamond

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Abstract

The emerging field of magnetometry based on NV centers opens a variety of new experimental perspectives, including the imaging of single nuclear spins on the nanoscale. However, in order to achieve exceptionally long NV electron spin coherence times and high sensitivities, the NV spin needs to be decoupled from unwanted interactions with the environment. This can be accomplished with dynamical decoupling sequences.

During the work for this thesis, multiple dynamical decoupling protocols were implemented and tested on NV centers in bulk diamond and nanodiamond. The theoretical part covers general NV properties before treating the behaviour of a free electron spin and finally applying this on the NV center. Then, the effect of different decoupling protocols are discussed. After that, the structure and concept of the setup will be explained. In the final part, the measurements will be presented. The execution of the decoupling sequences will be demonstrated and the data will be used to extract the spectral density function of the environment.

It was shown that all implemented dynamical decoupling sequences could enhance the coherence time. It was demonstrated that CPMG outperforms the other sequences on the given setup, achieving an improvement of up to a factor of 200 in the bulk diamond and 50 in nanodiamond. Finally, the examination of the spectral density functions of the spin bath gave a deeper insight in its coupling strength to the NV and its internal dynamics.

In the future, the limitations of the sequences will be further explored and other decoupling protocols will be tested. In addition to that, a better time and phase control has to be accomplished. These efforts will eventually lead to sensitivities high enough to detect small spin ensembles and even single molecular spins.

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1 Introduction

The human brain is one of the most investigated but still least understood subjects in scientific research. This comes as no surprise considering the huge variety of tasks it can perform efficiently and seemingly effortlessly: it constantly combines multiple sensory impressions and filters the most relevant of them to form a coherent image of the surroundings, it remembers information it has learned decades ago, it can produce the most complex thoughts and keep a whole organism working properly in the meantime. And despite the mayor improvement of processor performance and increasing interest in machine learning and artificial neural networks during the past couple of years, no technological implementation has even remotely managed to match the capability of the human brain.

The basis for its high functionality lies in the huge number of neurons - around 100 Billions[1] - and their interconnectivity: neural cells usually receive inputs from more than 10.000 other neurons[2]. Thus, in order to be able to understand how the brain works and possibly derive future applications from that, it is crucial to examine neural cells and study their characteristics.

Neural cells display a plethora of responses to their synaptic inputs. In general, neural activity can be divided into four mayor regimes: resting state, sub-threshold oscillations, spiking and bursting[3]. This work will focus on bursting neurons. These exhibit phases of repetitive spiking followed by periods of quiescence. A comparable behaviour was observed for Brownian Particles underlying bistable velocity dynamics[4][5], induced either via a velocity potential or movement in a biased cosine potential. In these systems, a specific range of parameters leads to diverging diffusion coefficients for vanishing noise intensity. This phenomenon is called "Giant Diffusion ". Applying this observation to neural cells, this could mean a large enhancement of the Signal-to-Noise Ratio through just a slight change in the system parameters. The goal of this thesis is to find out whether Giant Diffusion can be observed in a simple two-dimensional neuron model and which consequences this might have on the signal transmission, e.g. the Signal-to-Noise Ratio when the system is subject to an external stimulus.

2 Theory

2.1 Quantities of interest

In the context of Brownian Motion, there are two characteristic quantities: the ensemble of particles moves with a mean velocity

$$\langle v \rangle = \lim_{t \to \infty} \frac{\langle x(t) - x(0) \rangle}{t}$$
 (1)

and is subject to a diffusive spread around this average flow that can be described by the effective diffusion coefficient

$$D_{eff} = \lim_{t \to \infty} \frac{\langle x^2(t) \rangle - \langle x(t) \rangle^2}{2t}$$
 (2)

For the investigation of neuron models, a third quantity needs to be considered, namely the Fano factor:

$$F = \frac{\langle \Delta N^2(t) \rangle}{\langle N(t) \rangle}$$

In order to compare the neuron model with Brownian Particles, one may also define a Fano factor for mechanical systems:

$$F = \frac{2D_{eff}}{L\langle v \rangle}$$

where L can be chosen arbitrarily, e.g. a characteristic length of the system, so that F becomes dimensionless.

2.2 Giant Diffusion

The term "Giant Diffusion "is short for Giant Enhancement of (thermal) diffusion which was first observed around the turn of the millennium for Brownian Particles in a tilted periodic potential[6][7][8][9]. In general, these particles exhibit two stable velocity states. They can be "trapped"in a potential minimum - this is referred to as the locked state - or they can be in the running state. A particle gets into the running state if it has managed to overcome a hill and the frictional loss is low enough so that it is able to pass the adjacent hills as well. In the case of large friction or a strongly tilted potential, however, only one of these two states is present. If the potential is tilted in such a way that both states exist and the probabilities to be in either state are similar, many switchings between the states will occur. In the weak-noise-limit, half of the particles will be mainly in the locked state, while for the others the running state prevails. This behavior leads to diverging diffusion coefficients known as Giant Diffusion.

2.3 Giant diffusion of Brownian Particles

First observed by the botanist Robert Brown in 1828[10], the term *Brownian Motion* describes the irregular movement of particles in a viscous medium, whose apparently random changes of direction are caused by collisions with smaller particles or molecules.

Ordinary Brownian Motion obeys a simple linear Langevin-equation:

$$m\dot{v} = -\lambda v + \xi(t)$$

The evolution of the velocity v of the particle is affected by a linear friction term with coefficient λ and a random force $\xi(t)$.

In the following, two different systems with Brownian Motion dynamics exhibiting Giant Diffusion are presented. These were the motivation for my research on bursting neuron models.

2.3.1 Active Brownian Particles

Active Brownian Motion can be observed on small organisms, like bacteria or cells, which are able to move on their own. In order to model the behaviour of such an object, a more general friction term needs to be introduced into the Langevinequation:

$$\dot{v} = -f(v) + \xi(t)$$

Here, the noise was assumed to be additive and the mass was omitted due to clarity. An accurate description of the self-propulsion can be accomplished by choosing the function f in such a way that it attains negative values at small velocities and becomes greater than zero at large speed. Thus, at small velocities the particle will accelerate and with increasing velocity, regular friction will start to affect its motion. A system like this was studied by Lindner and Nicola in 2008[4]. They chose a cubic function for the friction term, $f(v) = v - v^3 + F$, allowing them to write the equation of motion in terms of a quartic velocity potential U(v):

$$\dot{v} = -U'(v) + \xi(t) \tag{3}$$

with $U(v) = \frac{1}{4}v^4 - \frac{1}{2}v^2 - Fv$.

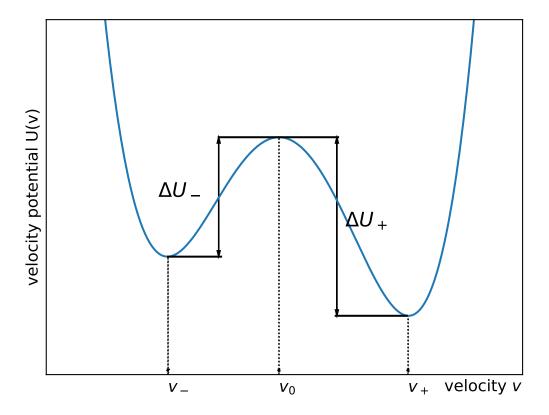


Figure 1: tilted velocity potential of an Active Brownian Particle

This potential shows two minima at v_{\pm} , representing the stable velocity states "forwards" and "backwards", and a maximum at v_0 . In order to transition from v_{\pm} into the other state, the particle needs to overcome a barrier of height $\Delta U \pm$. Their simulations revealed a certain region of bias forces F, in which giant diffusion occurred.

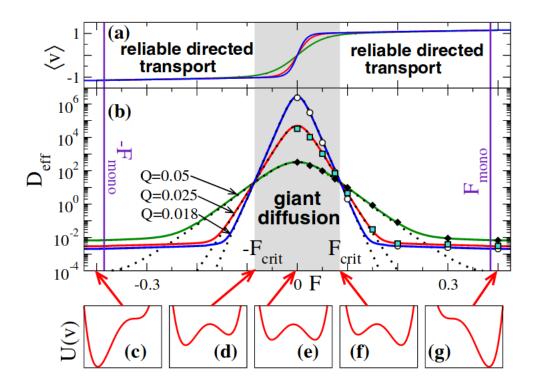


Figure 2: Simulation of velocity and effective diffusion coefficient for Active Brownian Particles underlying a tilted velocity potential, taken from [4]

Inside this region, the diffusion coefficients increase with decreasing noise intensity, while they decrease outside of this region. In other words, in the weak noise limit, the diffusion coefficients diverge in the critical region and vanish outside of it. The critical force lies at the border of this region and emerges from the intersection points of the diffusion coefficients for different noise levels. A simple criterion could be found for these intersection points: at the critical force, one potential barrier is twice as high as the other potential barrier. Furthermore, it is remarkable that the reliable directed transport which takes place outside of the critical region appears much earlier than the monostability of the velocity potential, which is a obviously only a primitive criterion for reliable transport in one direction. The mean velocity displays a more regular behavior. It is almost constant at a value less than zero up to small negative forces, then undergoes a sharp increase to a positive value and barely changes afterwards. They intersect as well, approximately at the position where the diffusion coefficient gets maximal.

2.3.2 Regular Brownian Particles in a tilted periodic potential

On their own, ordinary Brownian Particles do not exhibit bistable velocity dynamics which may lead to giant diffusion. But as mentioned before, this can be done by adding a periodic potential to the equation of motion:

$$\dot{v} = -\gamma v - U'(x) + \sqrt{2\gamma kT}\xi(t) \tag{4}$$

with $U(x) = -Fx - d\cos(x)$. This system was discussed with respect to giant diffusion in a paper by Lindner and Sokolov from 2016[5]. Now, in contrast to the Active Brownian Particle, the evolution of the system is not governed by a velocity potential, but by a spatial potential:

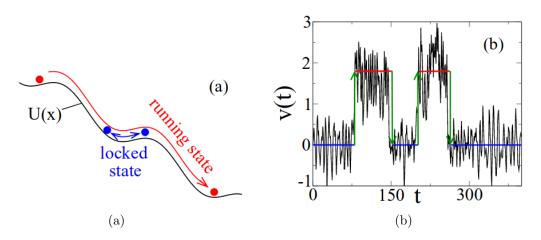


Figure 3: Figure (a) visualizes the motion of a Brownian Particle in a periodic potential, on the right one can see the bistable velocity dynamics. The oscillations thereby arise from local extrema of the potential.

Also for the Brownian Particles in a cosine potential, there was a finite range of bias forces, for which giant diffusion could be observed:

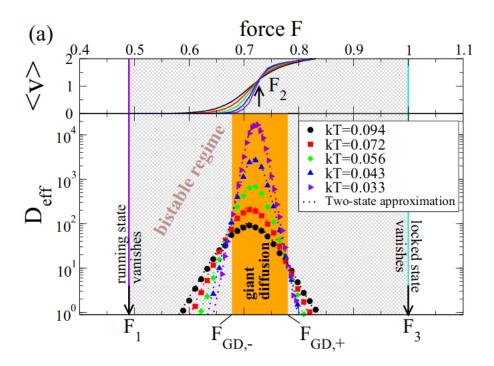


Figure 4: Simulation of velocity and effective diffusion coefficient for Brownian Particles in a tilted periodic potential, taken from [5]

Again, all curves of the diffusion coefficient intersect at two points and diverge in between those points for decreasing noise intensities while going to zero on the outside and the velocity curves intersect approximately at the maximum of the diffusion coefficient. And also here the region of giant diffusion is much smaller than the range of bias forces, where both states coexist. Two other variables that help characterize the system are the transition rates between the states, that is from the locked to the running state and vice versa. Even though there didn't exist

actual potential barriers, these turned out to obey an Arrhenius or Kramers law, respectively, as can be seen from an Arrhenius plot:

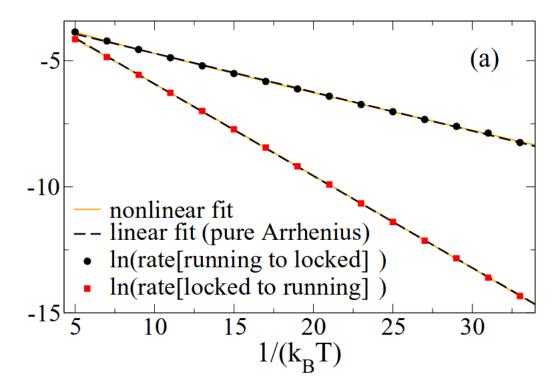


Figure 5: Fits of the transition rates with both an Arrhenius and a Kramers law, taken from [5]

In this example, the Arrhenius fit as well as the Kramers fit yield good agreements with the data. From these fits one can extract effective potential barriers. The relation found for the potential barriers of the Active Brownian Particle can be tested by plotting the effective barriers and twice their value:

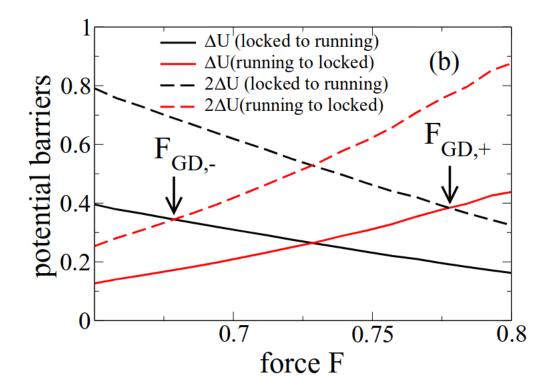


Figure 6: Plot of the effective potential barriers. The dotted curves are simply twice the solid curves of the same color. This plot is taken from [5]

The plot shows that the points where one potential barrier equals twice the other roughly correspond to the critical forces, so the criterion applies as well to this case, where no potential barriers were present and only effective barriers could be calculated.

2.4 Two-state theory

In the case of low noise intensity, the transition times between the locked state and the running state will be much shorter than the periods of time that the particle stays in one of the two states. That is why it is practical to describe the behavior of the system in this regime with a two-state model. The following derivation applies to the Brownian Particle in a tilted periodic potential. The transition rates are assumed to obey an Arrhenius law:

$$r_{\pm} = r_{0,\pm} \mathrm{e}^{-\frac{\Delta U_{\pm}}{D}}$$

where r_{-} denotes the transition rate from locked to running state, and r_{+} the rate for the other transition. ΔU_{\pm} is the corresponding potential barrier and D the noise intensity. The effective diffusion coefficient can be calculated from the velocity v_{0} in the running state and the transition rates:

$$D_{\text{eff}} = \frac{v_0^2 r_+ r_-}{(r_+ + r_-)^3}$$

The first task is to find the intersection points of the diffusion coefficients. At these points, the diffusion coefficients become independent of the noise intensity. It is

$$\begin{split} D_{\text{eff}} &= \frac{v_0^2 r_{0,+} r_{0,-} \mathrm{e}^{-\frac{\Delta U_+ + \Delta U_-}{D}}}{\left(r_{0,+} \mathrm{e}^{\frac{-\Delta U_+}{D}} + r_{0,-} \mathrm{e}^{\frac{-\Delta U_-}{D}}\right)^3} \\ &= \frac{v_0^2 r_{0,+} r_{0,-}}{\left(r_{0,+} \mathrm{e}^{-\frac{3\Delta U_+ - \Delta U_+ - \Delta U_-}{3D}} + r_{0,-} \mathrm{e}^{-\frac{3\Delta U_- - \Delta U_+ - \Delta U_-}{3D}}\right)^3} \\ &= \frac{v_0^2 r_{0,+} r_{0,-}}{\left(r_{0,+} \mathrm{e}^{-\frac{2\Delta U_+ - \Delta U_-}{3D}} + r_{0,-} \mathrm{e}^{-\frac{2\Delta U_- - \Delta U_+}{3D}}\right)^3} \end{split}$$

In the limes $D \to 0$, $\Delta U_+ > U_-$ the first term in the denominator vanishes, resulting in:

$$D_{\text{eff}} = \frac{v_0^2 r_{0,+}}{r_{0,-}^2} e^{-\frac{\Delta U_+ - 2\Delta U_-}{D}}$$

Under the assumption that the prefactors change slowly in comparison to the exponential function, the following condition arises:

$$\Delta U_{+} = 2\Delta U_{-}$$

Due to symmetry of the problem, the opposing case $D \to 0, \Delta U_+ < U_-$ yields:

$$\Delta U_{-} = 2\Delta U_{+}$$

In both cases, one potential barrier is twice as high as the other one.

Next, we will examine whether the Fano factor displays similar features in the weak noise limit. As

$$F = \frac{2D_{\text{eff}}}{L\langle v \rangle}$$

an expression for the average velocity is required to compute the Fano factor. Taking into account that the average velocity is zero when the particle is in the locked state, one finds the following formula for the total mean velocity:

$$\langle v \rangle = v_0 \frac{r_-}{r_+ + r_-}$$

Therefore

$$F = \frac{2v_0 r_+}{(r_+ + r_-)^2} = \frac{2v_0 r_{0,+} e^{\frac{-\Delta U_+}{D}}}{\left(r_{0,+} e^{\frac{-\Delta U_+}{D}} + r_{0,-} e^{-\frac{\Delta U_-}{D}}\right)^2}$$

In the limes $D \ll 1$ there are again two solutions. For $\Delta U_+ > \Delta U_-$:

$$F = \frac{2v_0 r_{0,+}}{r_{0,-}^2} e^{-\frac{\Delta U_+ - 2\Delta U_-}{D}} \to \Delta U_+ = 2\Delta U_-$$

as well as for $\Delta U_{+} < \Delta U_{-}$:

$$F = \frac{2v_0}{r_{0,+}} e^{-\frac{\Delta U_+ - 2\Delta U_+}{D}} \to \Delta U_+ = 0$$

The intersection point for $\Delta U_+ > \Delta U_-$ stays the same while at the other critical point the potential barrier from running to locked state needs to vanish. As the latter condition violates the requirements for the application of the two-state theory - because only one state would exist in this case - the second intersection point can't be determined via this two-state model.

3 Giant diffusion in a bursting neuron model

3.1 Brownian motion and neuronal models

Brownian motion in periodic potentials has numerous applications among which one can find superionic conduction, rotation of a dipole in a static field or the description of a Josephson Tunneling junction[11]. However, apart from these mechanical examples, Brownian motion in periodic potentials is also suited to describe a bursting neuron. If one counts every time the particle crosses a hill as a spike, the running state can be associated with tonic firing and the locked state with a stable equilibrium point. Because of the random noise, transition between the states will occur and the sustained spiking will be eventually terminated so that there is only a finite number of spikes within each burst. The position of the Brownian Particle then corresponds to the spike count of the neuron and its velocity to the firing rate. Thus, based on the similarities to Brownian motion, we expect to find a weak noise behavior comparable to giant diffusion in bursting neurons as well.

3.2 Neuronal bursting

Depending on its physiology and the properties of the stimulus, a neuron doesn't always fire a single spike. A series of multiple spikes in a short time interval that is followed by a period of quiescence is called a burst[2]. Typically, bursting results from the interplay between two subsystems: a fast subsystem, that is responsible for the generation of the spikes within a burst, and a slow subsystem that modulates the bursting pattern and eventually terminates sustained spiking. However, a bursting neuron model that implements these slow and fast dynamics would at least have to be three-dimensional, as there would be a variable for the membrane voltage as well as for the fast and slow oscillations. One way to realize a bursting two-dimensional model and to make use of the various methods of phase plane analysis is to introduce noise into the system. Considering that any neuron is subject to some kind of noise, this is a justified assumption and was even proposed by Izhikevich as a way to make two-dimensional neuronal models burst[2].

3.3 The bursting neuron model

The main focus of this thesis lies on the study of the $I_{Na,p} + I_K$ -model, the persistent sodium plus potassium model with additive noise:

$$C\dot{V} = I - g_L(V - E_L) - g_{Na}m_{\infty}(V)(V - E_{Na}) - g_Kn(V - E_K) + \sqrt{2D}\xi(t)$$
 (5)

$$\dot{n} = (n_{\infty}(V) - n)/\tau(V) \tag{6}$$

Here, V denotes the mambrane voltage, C is the capacitance, I is the bias current, g_i are conductances and E_i the Nernst equilibrium potentials. The overall noise intensity is D. Lastly, m_{∞} is the activation variable of the instantaneous Na^+ current, while n governs the variation of the slower K^+ current. The steady-state activation functions are approximated by the Boltzmann-function:

$$f_{\infty}(V) = \frac{1}{1 + \exp\{(V_{1/2} - V)/k\}}$$

At $V_{1/2}$, the activation function has the value 1/2, and k is the slope factor determining the steepness around $V_{1/2}$ - a smaller value of k leads to a more abrupt change

of f_{∞} . This approximation was suggested by Izhikevich [2].

The fastest neural oscillations in the human brain are gamma waves with frequencies in the range between 25 and 100 Hz[12][13]. Similar values can also be found in different papers about bursting neurons[14][15]. Therefore, the parameters were chosen such that the frequency in the bursting state was about 70 Hz. The exact values used in the simulations were:

$$C = 1$$
, $g_L = 0.3$, $E_L = -80$, $g_{Na} = 1$, $E_{Na} = 60$, $g_K = 0.4$, $E_K = -90$.

Instantaneous Na^+ current:

$$k_m = 14, V_{1/2,m} = -18.$$

 K^+ current:

$$k_n = 5, V_{1/2,n} = -25, \tau(V) = \text{const} = 3.$$

3.3.1 Phase plane analysis

For a system that depends on the evolution of two state variables, in this case V and n, some qualitative and quantitative analysis can be carried out in the phase plane. A neat way to obtain information about an unknown system is to calculate its nullclines. The nullclines are curves in the phase plane, where one of the state variables remains constant. Thus, the V-nullcline is defined by the condition $\dot{V}=0$ and the n-nullcline follows from $\dot{n}=0$. By crossing one of the nullclines, the system changes its direction with respect to the corresponding variable. As a consequence, each nullcline separates the phase space into two regions where one variable evolves in opposite directions. Taken together, the nullclines define four different regions of directions: one region each where both variables decrease or increase and two regions where one variable increases and the other decreases. Depending on the specific shape of the nullclines, these do not necessarily have to be coherent.

The V-nullcline can be obtained by setting the left side of equation (5) to zero. In the V-n-plane, it can then be described by the function

$$n(V) = \frac{I - g_L(V - E_L) - g_{Na} m_{\infty}(V)(V - E_{Na})}{g_K(V - E_K)}$$
(7)

The n-nullcline is just

$$n(V) = n_{\infty}(V) \tag{8}$$

The nullclines of the $I_{Na,p} + I_K$ -model are shown in figure 7.

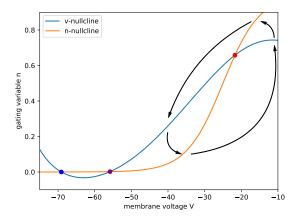


Figure 7: Nullclines of the $I_{Na,p} + I_K$ -model. The equilibrium points are marked with dots: the red dot denotes a stable equilibrium, the blue dot an unstable focus and the purple dot a saddle point

A second aspect of the nullclines are their intersection points. As both state variables remain constant when the nullclines intersect, these points are equilibrium points.

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Mir ist bekannt, dass bei Verstößen gegen diese Grundsätze ein Verfahren wegen
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