

CS-736 Assignment: Statistical Image Modeling, Image Denoising

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1. (25 points) Bayesian Denoising of a Phantom Magnetic Resonance Image.

Get the 2D noiseless image and the 2D noisy image in the “data” folder.

Implement a **maximum-a-posteriori Bayesian image-denoising** algorithm that uses a suitable noise model (i.i.d. Gaussian or independent Rician) coupled with a MRF prior that uses a 4-neighbor neighborhood system (each pixel has 4 neighbors: left, right, up, down; the neighborhood wraps around at image boundaries) that has cliques of size *no* more than 2.

Use gradient ascent optimization with dynamic step size; implementing a fixed step size isn't acceptable. Ensure that the value of the objective function, i.e., the log posterior, at each iteration increases. Use the noisy image as the initial estimate.

Use 3 different MRF priors where the potential functions $V(x_i, x_j) := g(x_i - x_j)$ underlying the MRF penalize the difference between the neighboring voxel values x_i, x_j as follows (see class notes for details). You may rely on the “circshift()” function in Matlab when computing differences between every pixel in the image and its neighbors.

Introduce a parameter $\alpha \in [0, 1]$ to control the weighting between the prior (weight α) and the likelihood (weight $1 - \alpha$).

Specifically, implement the following functionality as part of the denoising algorithm:

(a) (2 points)

A suitable noise model. You don't need the noise level because that parameter can be absorbed in $1 - \alpha$ that you'll tune manually (Tuning α essentially manipulates the noise level, in case of the likelihood. So we can ignore the noise level σ when tuning α manually. Use $\sigma = 1$).

(b) (2 points)

MRF prior: Quadratic function: $g_1(u) := |u|^2$.

(c) (2 points)

MRF prior: Discontinuity-adaptive Huber function: $g_2(u) := 0.5|u|^2$, when $|u| \leq \gamma$ and $g(u) := \gamma|u| - 0.5\gamma^2$, when $|u| > \gamma$, where $0 < \gamma < \infty$ is a constant.

(d) (2 points)

MRF prior: Discontinuity-adaptive function: $g_3(u) := \gamma|u| - \gamma^2 \log(1 + |u|/\gamma)$, where $0 < \gamma < \infty$ is a constant.

For each MRF prior, manually tune the parameters α and γ (where applicable) to denoising the noisy image in order to achieve the least possible relative root-mean-squared error (RRMSE). The RRMSE for 2 images A and B is defined as :

$$\text{RRMSE}(A, B) = \sqrt{\sum_p (|A(p)| - |B(p)|)^2} / \sqrt{\sum_p |A(p)|^2}$$
, where the summation is over all pixels p ; always use the noiseless image as A .

Report the following:

(a) (0 point)

Report the RRMSE between the noisy and noiseless images.

(b) (8 points)

Report the optimal values of the parameters and the corresponding RRMSEs for each of the 3 denoising algorithms. For each optimal parameter value reported (for each of the 3 denoising algorithms), give evidence of the optimality of the reported values by reporting the RRMSE values for two nearby parameter values (around the optimal) at plus/minus 20% of the optimal value. That is, if a^*, b^* are the optimal parameter values, then report:

$a^*, b^*, \text{RRMSE}(a^*, b^*),$

$\text{RRMSE}(1.2a^*, b^*), \text{RRMSE}(0.8a^*, b^*),$

$\text{RRMSE}(a^*, 1.2b^*), \text{RRMSE}(a^*, 0.8b^*).$

(Tip: the optimal values for α might be very close to extreme limits of the allowed range. Be aware of that possibility.)

(c) (6 points)

Show the following 5 images (at each pixel, show the magnitude of the pixel value; use a jet colormap) in the report using exactly the same colormap (i) Noiseless image, (ii) Noisy image,

(iii) Image denoised using quadratic prior $g_1(\cdot)$ and optimal parameter tuning;

(iv) Image denoised using Huber prior $g_1(\cdot)$ and optimal parameter tuning;

(v) Image denoised using discontinuity-adaptive prior $g_3(\cdot)$ and optimal parameter tuning.

(d) (3 points)

Show the plots of the objective-function values (vertical axis) versus iteration (horizontal axis) corresponding to each of the 3 denoised results in (iii), (iv), and (v) above.

2. **(9=6+3 points) Bayesian Denoising of a Brain Magnetic Resonance Image.**

Repeat the same task for the brain MRI image in the “data” folder.

Show the images and the plots.

3. (9=6+3 points) Bayesian Denoising of a RGB Microscopy Image.

Repeat the same task for the microscopy image in the “data” folder (assuming a Gaussian noise model as an approximation), but with the following MRF prior functions:

(A) where the penalty between two vector-valued neighboring pixels is the squared-L2-norm of their vector difference;

(B) where the penalty between two vector-valued neighboring pixels is the L2 norm of their vector difference;

(C) where the penalty between two vector-valued neighboring pixels is the (Huber-regularized) L1 norm of their vector difference.

- (a) (6 points) Show the following 5 images (at each pixel, show the magnitude of the pixel value; use a jet colormap) in the report using exactly the same colormap (i) Noiseless image, (ii) Noisy image, (iii) Image denoised using prior-A and optimal parameter tuning, (iv) Image denoised using prior-B and optimal parameter tuning, (v) Image denoised using prior-C and optimal parameter tuning.

In which of the three cases (i.e., A,B,C) do you observe edge preservation ? and why ?

- (b) (3 points) Show the plots of the objective-function values (vertical axis) versus iteration (horizontal axis) corresponding to each of the 3 denoised results above.

4. (25 points) Dictionary Learning on Image Patches, Followed by Image Denoising.

Get the 2D chest-CT image in the “data” folder.

Consider a dictionary matrix D with K columns as its atoms, where the k -th column d_k , for any k , has $\|d_k\|_2 \leq 1$ (hard constraint).

Consider the following dictionary learning formulation for some set of image patches $\{x_i\}_{i=1}^I$, under the hard constraint stated above:

$$\arg \min_D \min_r \sum_{i=1}^I \|x_i - Dr_i\|_2^2 + \lambda \|r_i\|_p^p,$$

where each r_i is a column vector (of length K) containing the coefficients used in the representation of image patch x_i , and $p > 0$ parameterizes the norm/quasi-norm of the vector r_i .

(a) (9 points)

Implement a function to learn the dictionary D for image patches of size 8×8 pixels. The dictionary D should have the number of atoms $K = 64$. Your optimization algorithm should be the same for any suitable choice of p .

For computational efficiency, the learning must only use a subset of image patches that have a sufficiently large variance of intensities within the patch (e.g., avoiding constant-intensity patches). Nevertheless, the final dictionary must indeed be able to model and fit all kinds of patches. With these design motivations, engineer a strategy to create the subset of patches $\{x_i\}_{i=1}^I$ (within the given image) that will be used to learn D , and justify your strategy.

(b) (6 points)

Use your function to learn four different dictionaries for values of $p = 2, p = 1.6, p = 1.2, p = 0.8$.

• (2 points)

In each of the 4 cases, during the optimization process, show the graph of the objective function versus iterations.

• (2 points)

In each of the 4 cases, before and after the optimization process, show the atoms used as the initial estimate (must be same for all cases) and the optimal estimates. Describe any trend that you observe.

• (2 points)

In each of the 4 cases, after the optimization process, show the histogram of coefficients within each r_i , pooled across all r_i . Describe and justify the trend that you (expect to) observe.

(c) (10 points)

• (2 points)

Given the 2D chest-CT image, simulate a noisy (or noisier) version by introducing i.i.d. Gaussian zero-mean noise of standard deviation equaling 10% of the intensity range in the given image.

• (4 points)

You want to use the learned dictionary for $p = 0.8$ to denoise the simulated noisy image (not just a subset of its patches). Propose an optimization problem for the same, and implement a function to compute an optimal estimate of the denoised image.

• (2 points)

During the optimization process, show the graph of the objective function versus iterations.

• (2 points)

Show the simulated noisy image, the denoised image, and the original/given image.