

HOMEWORK #1

Course: MCEN 5228 – Modeling of Human Movement

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Date: 02/09/2021

Q1)	<ul style="list-style-type: none"> a) Biceps Brachii: elbow flexion b) Triceps (all heads): elbow extension c) Anterior Deltoid: shoulder flexion d) Posterior Deltoid: shoulder extension e) Pectoralis Major: glenohumeral adduction f) Rectus Femoris: hip flexion g) Vastus Lateralis: knee extension h) Vastus Medialis: knee extension i) Vastus Intermedius: knee extension j) Semitendinosus: hip extension k) Semimembranosus: hip extension l) Biceps Femoris: knee flexion m) Gastrocnemius: ankle plantarflexion n) Soleus: ankle plantarflexion o) Tibialis Anterior: ankle dorsiflexion p) Gluteus Maximus: hip extension q) Gluteus Medius: hip abduction
Q2)	<ul style="list-style-type: none"> a) Movement in Sagittal plane: Walking b) Movement in Transverse plane: Twisting lunges c) Movement in Frontal plane: Jumping jack exercises

$$Q3) \Rightarrow \ddot{x}_m + \frac{b}{m} \dot{x}_m + \frac{k_m}{m} x_m = 0$$

This is a homogeneous linear second-order differential equation. The general solution of the differential equation is

$$x(t) = C \exp(\lambda_1 t) + D \exp(\lambda_2 t)$$

where C and D are arbitrary constants.

Let $p = b/m$ and $q = k_m/m$.

$$\Rightarrow \frac{d^2 x_m}{dt^2} + p \frac{dx_m}{dt} + \frac{k_m}{m} x_m = 0$$

$$\Rightarrow \frac{d^2 x_m}{dt^2} + p \frac{dx_m}{dt} + q x_m = 0$$

Auxiliary equation for this differential equation is,

$$\Rightarrow \lambda^2 + p\lambda + q = 0$$

The roots for the auxiliary equation are

$$\lambda_1 = -\frac{p + \sqrt{p^2 - 4q}}{2} \quad \text{and} \quad \lambda_2 = -\frac{p - \sqrt{p^2 - 4q}}{2}$$

$$\Rightarrow \lambda_1 = \frac{-(b/m) + \sqrt{(b^2/m^2) - (4k_m/m)}}{2} \quad \text{and}$$

$$\lambda_2 = \frac{-(b/m) - \sqrt{(b^2/m^2) - (4k_m/m)}}{2}$$

$$\therefore x_m(t) = C \exp\left[-t(\sqrt{b^2 - 4k_m/m} + b)/2m\right] \\ + D \exp\left[t(\sqrt{b^2 - 4k_m/m} - b)/2m\right]$$

$$Q4) \Rightarrow \frac{dx(t)}{dt} = 5x(t) + 3, \text{ where } x(0) = 0$$

$$\Rightarrow \frac{dx(t)}{5x(t) + 3} = dt$$

$$\Rightarrow \int \frac{dx(t)}{5x(t) + 3} = \int dt + C_1$$

$$\text{Let, } 5x(t) + 3 = u$$

$$\text{Then, } 5dx(t) = du \Rightarrow dx(t) = du/5$$

Substituting back in our equation, we get,

$$\Rightarrow \int \frac{du/5}{u} = \int dt + C_1$$

$$\Rightarrow \frac{1}{5} \ln u = t + C_1$$

$$\Rightarrow u = e^{5t} \cdot e^{C_1} = e^{5t} \cdot C_2 \quad (\text{where, } C_2 = e^{C_1})$$

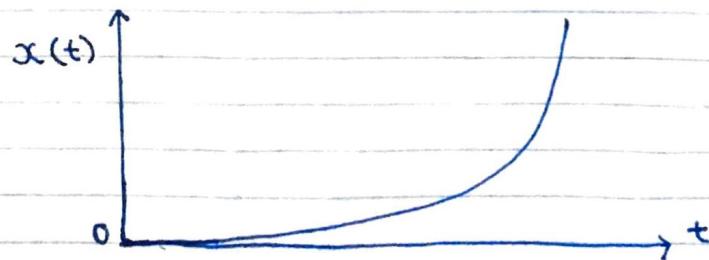
$$\Rightarrow 5x(t) + 3 = C_2 e^{5t}$$

$$\Rightarrow x(t) = (C_2 e^{5t} - 3)/5$$

$$\Rightarrow x(t) = \frac{C_2 e^{5t}}{5} - \frac{3}{5} = C_3 e^{5t} - \frac{3}{5} \quad (\text{where, } C_3 = \frac{C_2}{5})$$

$$\text{Also, } x(0) = 0 = C_3 e^0 - \frac{3}{5} \Rightarrow C_3 = 3/5$$

$$\therefore x(t) = \frac{3}{5} (e^{5t} - 1)$$



Q5) Given two vectors \vec{x} and \vec{y} , $\vec{x} \times \vec{y}$ is a vector that is perpendicular to both \vec{x} and \vec{y} .

$$\therefore \text{Let, } \vec{w} = \vec{x} \times \vec{y}$$

$$\Rightarrow \vec{w} = \begin{vmatrix} \hat{i} & \hat{j} & \hat{k} \\ 4 & 3 & 5 \\ -1 & -5 & 3 \end{vmatrix}$$

$$\Rightarrow \vec{w} = \hat{i}(9 - (-25)) - \hat{j}(12 - (-5)) + \hat{k}(-20 - (-3))$$

$$\Rightarrow \vec{w} = 34\hat{i} - 17\hat{j} - 17\hat{k}$$

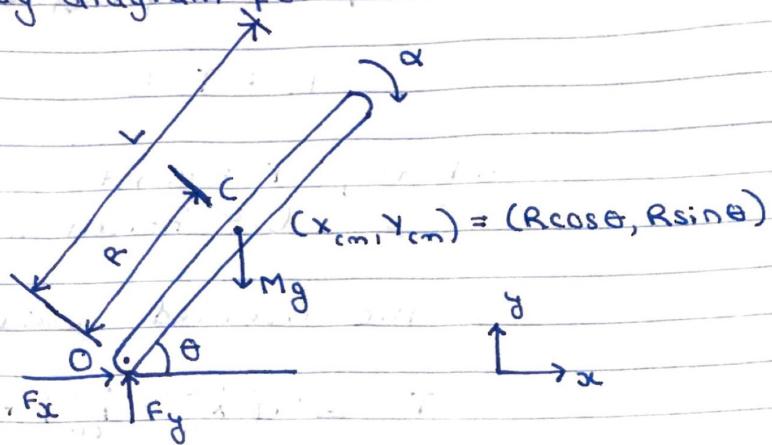
Unit vector, \hat{w} is given by, $\frac{\vec{w}}{\|\vec{w}\|}$

$$\Rightarrow \|\vec{w}\| = \sqrt{(34)^2 + (-17)^2 + (-17)^2} = 17\sqrt{6}$$

$$\Rightarrow \hat{w} = \frac{34\hat{i} - 17\hat{j} - 17\hat{k}}{17\sqrt{6}} = \frac{\sqrt{6}}{3}\hat{i} - \frac{1}{\sqrt{6}}\hat{j} - \frac{1}{\sqrt{6}}\hat{k}$$

Hence, required vector, $\hat{w} = \left(\frac{\sqrt{6}}{3}, -\frac{1}{\sqrt{6}}, -\frac{1}{\sqrt{6}} \right)$

Q6) \Rightarrow Free body diagram for the inverted pendulum:-



Q7) \Rightarrow Method 1) \Rightarrow Using Newtonian Mechanics :

We know that, $M_o = I_o \alpha$
(where, M_o is moment about point O)
 $\Rightarrow M_o = Mg(R\cos\theta)$

Also, $I_o = I_{cm} + MR^2$

$\therefore M_o = MgR\cos\theta = (I_{cm} + MR^2)\alpha$

$$\Rightarrow \boxed{\alpha = \frac{MgR\cos\theta}{(I_{cm} + MR^2)}}$$

Method 2) \Rightarrow Using Lagrangian Mechanics:

$$L = T - U$$

where, T = Kinetic energy

U = Potential energy

For the inverted pendulum problem,

$$T = \frac{1}{2} M (\dot{x}_{cm}^2 + \dot{y}_{cm}^2) + \frac{1}{2} I_{cm} \dot{\theta}^2$$

$$\Rightarrow T = \frac{1}{2} M (R^2 \dot{\theta}^2 \cos^2 \theta + R^2 \dot{\theta}^2 \sin^2 \theta) + \frac{1}{2} I_{cm} \dot{\theta}^2$$

$$\Rightarrow T = \frac{1}{2} M R^2 \dot{\theta}^2 + \frac{1}{2} I \dot{\theta}^2$$

$$U = Mg(R \sin \theta) = MgR \sin \theta$$

$$\text{So, } L = T - U$$

$$\Rightarrow L = \frac{1}{2} M R^2 \dot{\theta}^2 + \frac{1}{2} I \dot{\theta}^2 - MgR \sin \theta$$

According to Euler-Lagrange equations, or
Lagrange's equations of the second kind,

$$\frac{\partial L}{\partial q} - \frac{d}{dt} \left(\frac{\partial L}{\partial \dot{q}} \right) = 0 \quad \text{--- (A)}$$

$$\text{So, } \frac{\partial L}{\partial \theta} = -MgR \cos \theta \quad \text{--- (i)}$$



$$\text{Also, } \frac{\partial L}{\partial \dot{\theta}} = \frac{1}{2} MR^2 2\ddot{\theta} + \frac{1}{2} I 2\dot{\theta} = \dot{\theta}(MR^2 + I)$$

$$\therefore \frac{d}{dt} \left(\frac{\partial L}{\partial \dot{\theta}} \right) = \ddot{\theta}(MR^2 + I) \quad \textcircled{i}$$

Substituting \textcircled{i} and \textcircled{ii} in \textcircled{A} , we get,

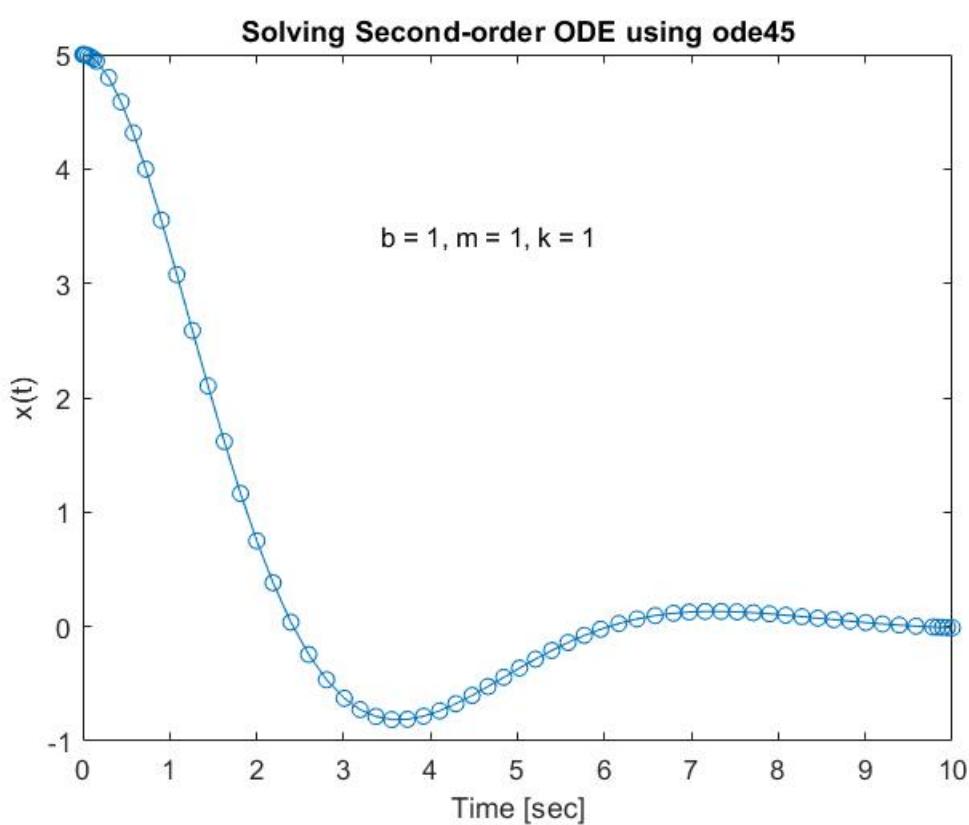
$$\Rightarrow -MgR\cos\theta - \ddot{\theta}(MR^2 + I) = 0$$

$$\Rightarrow \ddot{\theta}(MR^2 + I) = -MgR\cos\theta$$

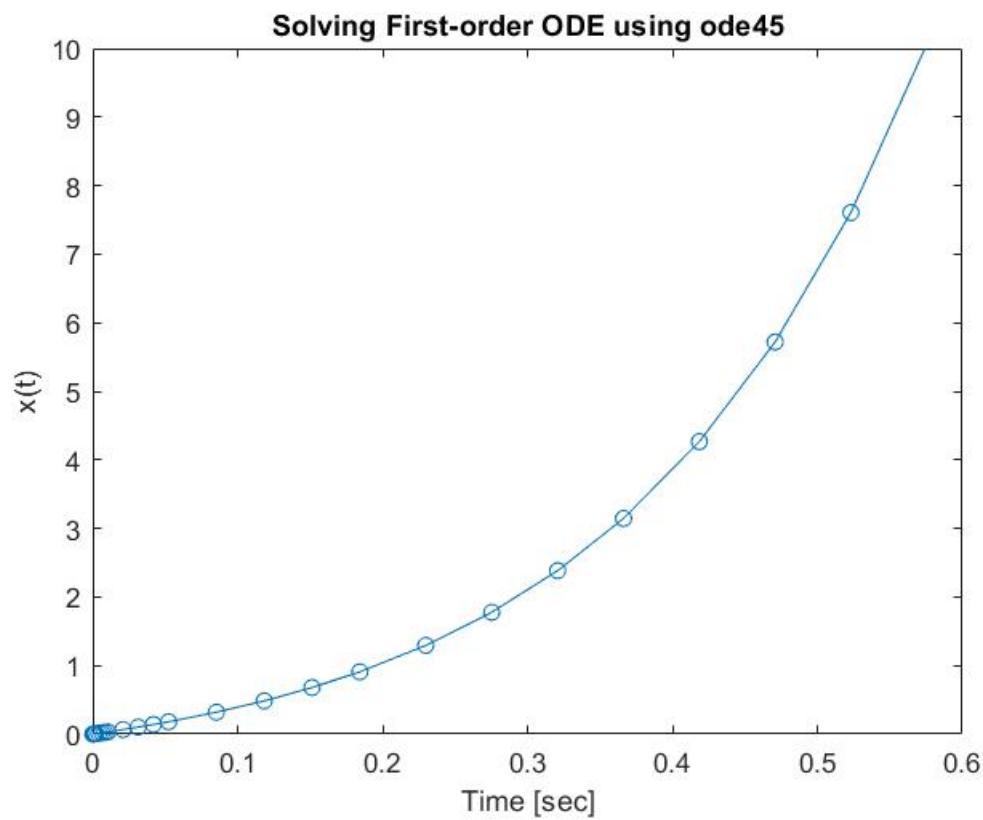
$$\Rightarrow \boxed{\ddot{\theta} = \frac{-MgR\cos\theta}{(I + MR^2)}}$$

Q8) According to Hooke's law, the displacement or size of deformation is directly proportional to the deforming force or load for relatively small deformations of an object. The equation for Hooke's law is, $F = k*x$, where F is the force, x is the length of extension/compression and k is a constant of proportionality known as the spring constant. Hooke's law can represent muscles and tendons (the tissue connecting muscle to bone). It is because of the elasticity of biological substances and muscle fibers. Some tendons have a high collagen content so there is relatively little strain, on the other hand, support tendons can have strain up to 10%.

Q9) a)

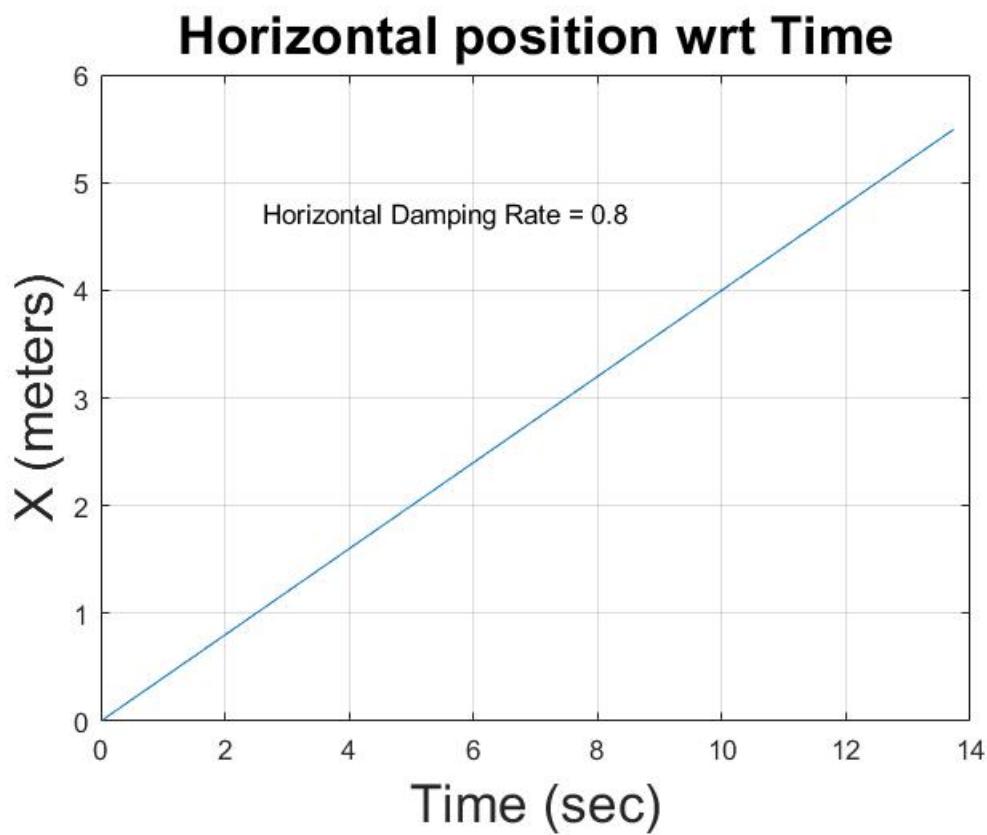


b)

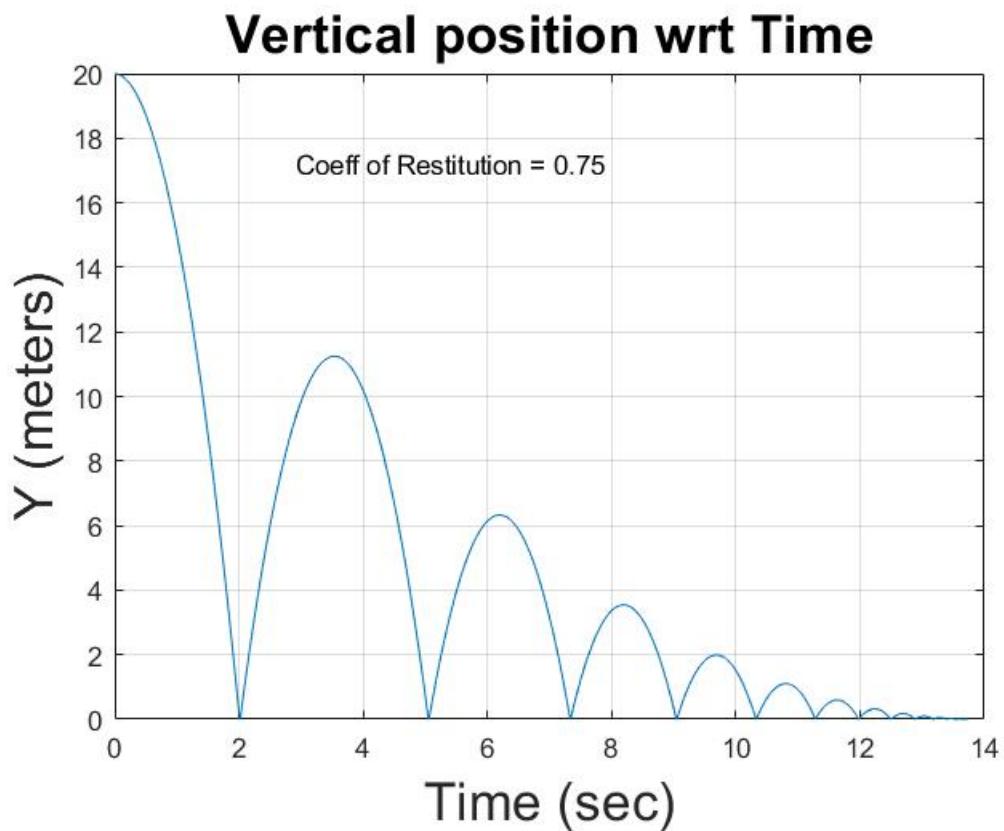


Q10)

a)



b)



c)

