

An Automated Microfluidic Paper-Based Analytical Device for Chemiluminescence Immunoassay

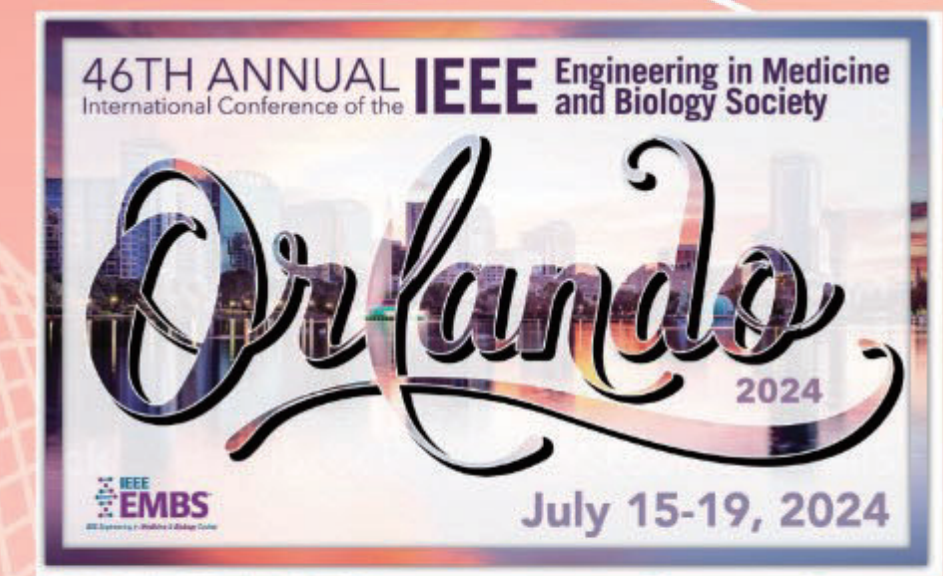
Jihong Sun^{1,2}, Sixuan Duan^{1,2}, Ruiqi Yong¹, Hang Yuan¹,
Sanli Liu^{1,2}, Kai Hoettges², Junhui Zhu³, Mark Leach^{1,2}, Pengfei Song^{1,2,*}

¹ School of Advanced Technology, Xi'an Jiaotong-Liverpool University, Suzhou, China

² Department of Electrical and Electronic Engineering, University of Liverpool, Liverpool, UK

³ School of Electronic and Information Engineering, Suzhou University of Science and Technology, Suzhou, China

* Contact: pengfei.song@xjtlu.edu.cn



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ABSTRACT

This paper introduces a highly integrated microfluidic paper-based analytical device (μ PAD) with a reliable and programmable rotary valve and automated injection system. By controlling the rotation of the valve, different regions on the μ PAD can be connected or disconnected, allowing effective reagent transport to the test zone. To address the limitations of traditional chemiluminescent immunoassays (CLIA), which require expensive equipment and extensive manual operations, we use a smartphone to read the results and control the device. As a proof-of-concept, we detected rabbit IgG under optimized experimental conditions, achieving a limit of detection of 3.58 pM.

INTRODUCTION

Chemiluminescence (CL) on microfluidic paper-based analytical devices (μ PADs) offers low limits of detection (LOD) and high reproducibility [1].

- Traditional CL measurements require expensive photodetectors (e.g., photomultiplier tubes and charge-coupled devices).
- Smartphones, equipped with high-resolution cameras and powerful computing capabilities, simplify CL detection [2].
- Our method offers comparable sensitivity to chemiluminescence immunoassay (CLIA) using magnetic nanoparticles (4 pM).



RESULTS

Detected rabbit IgG by direct ELISA on our μ PAD (Fig. 4): LOD = 3.58 pM; $R^2 = 0.997$

- Optimized experimental conditions (H_2O_2 concentration at 0.1 M, HRP-conjugated antibody concentration at 150 μ g/mL, and plasma treatment time of 4 minutes).

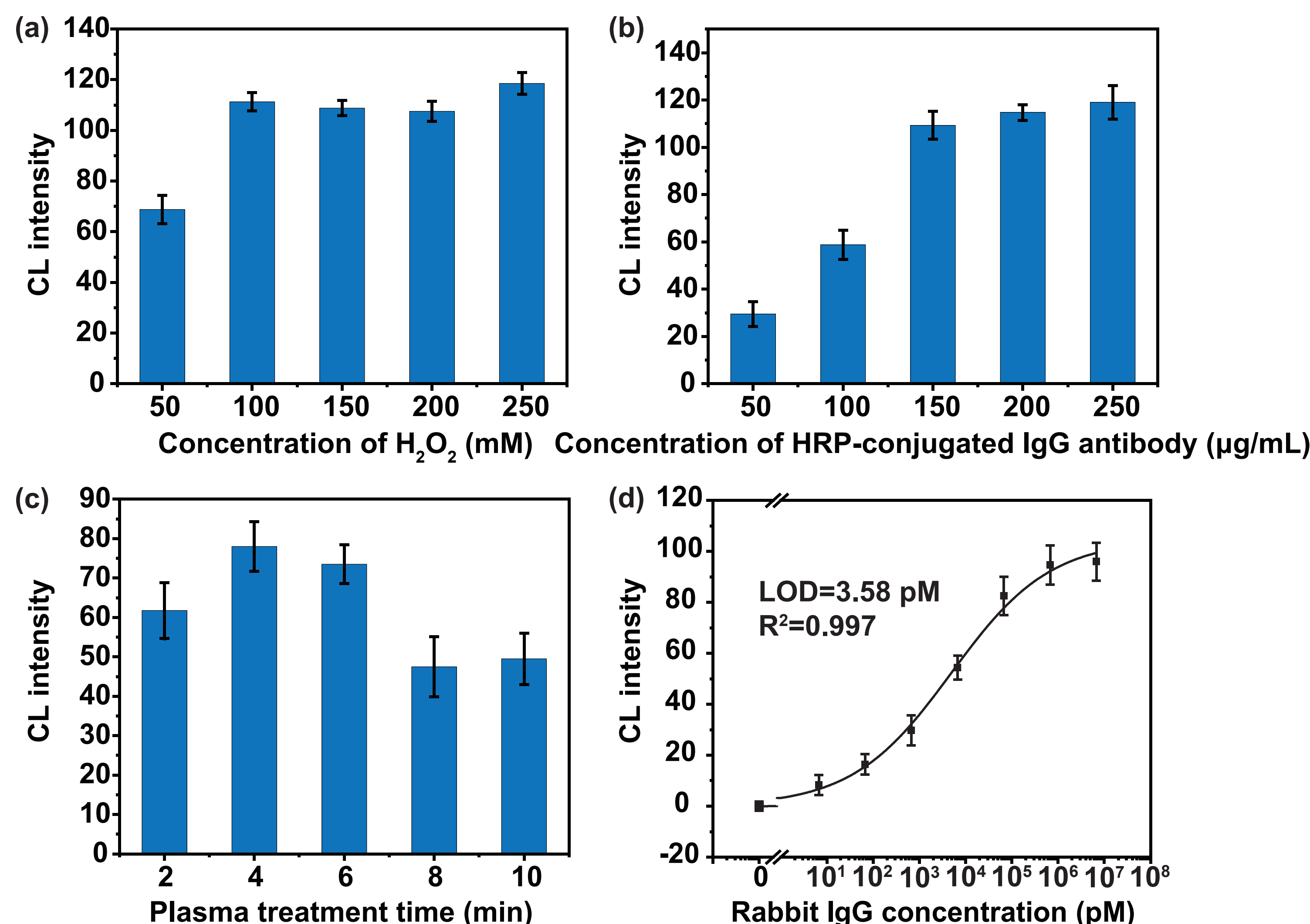


Fig. 4. (a-c) Optimized experimental conditions include the concentrations of H_2O_2 and HRP-conjugated IgG antibody, and the oxygen plasma treatment time. (d) Calibration curve of CL intensity vs rabbit IgG concentration ($N=5$).

CONCLUSION

This paper introduces a smartphone-based μ PAD for automated CLIA. As a proof-of-concept, the LOD of rabbit IgG on this μ PAD reached 3.58 pM.

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References:

- [1] J. Ma et al., "Smartphone-based chemiluminescence detection of aflatoxin B1 via labelled and label-free dual sensing systems," *Food Chemistry*, vol. 413, p. 135654, 2023.
- [2] A. Roda et al., "Integrating biochemiluminescence detection on smartphones: mobile chemistry platform for point-of-need analysis," *Analytical Chemistry*, vol. 86, no. 15, pp. 7299-7304, 2014.

METHODS

- Our device introduces pre-mixed reagents at precise intervals, including luminol, H_2O_2 and enhancers, during the detection process through a highly integrated injection system (Fig. 1).

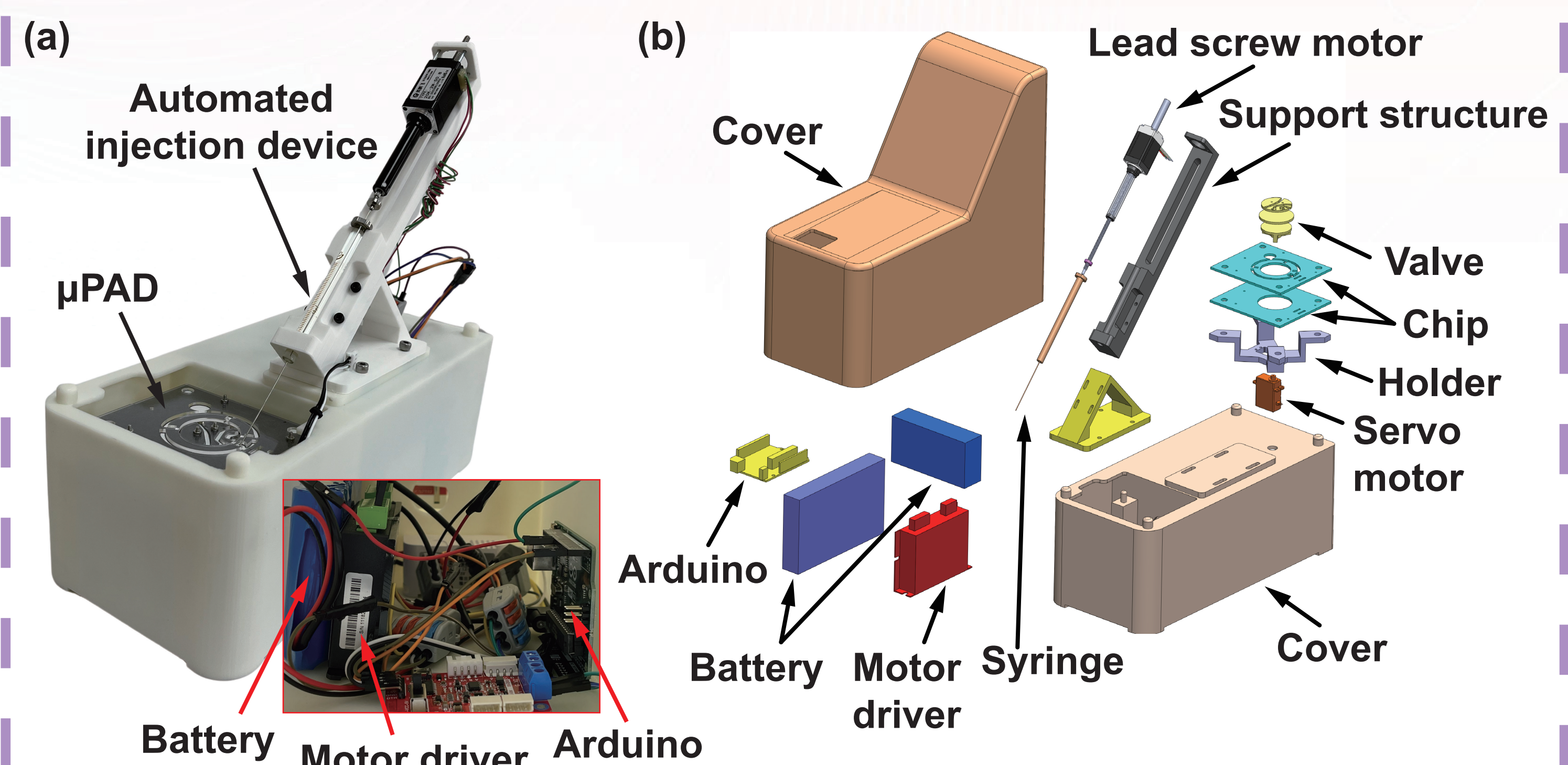


Fig. 1. (a) The photo of the developed device and its internal components. (b) Exploded diagram of the entire system.

- Captured photos of CL results using a smartphone exposed for 30 seconds, and analyzed CL intensity using ImageJ (Fig. 2).

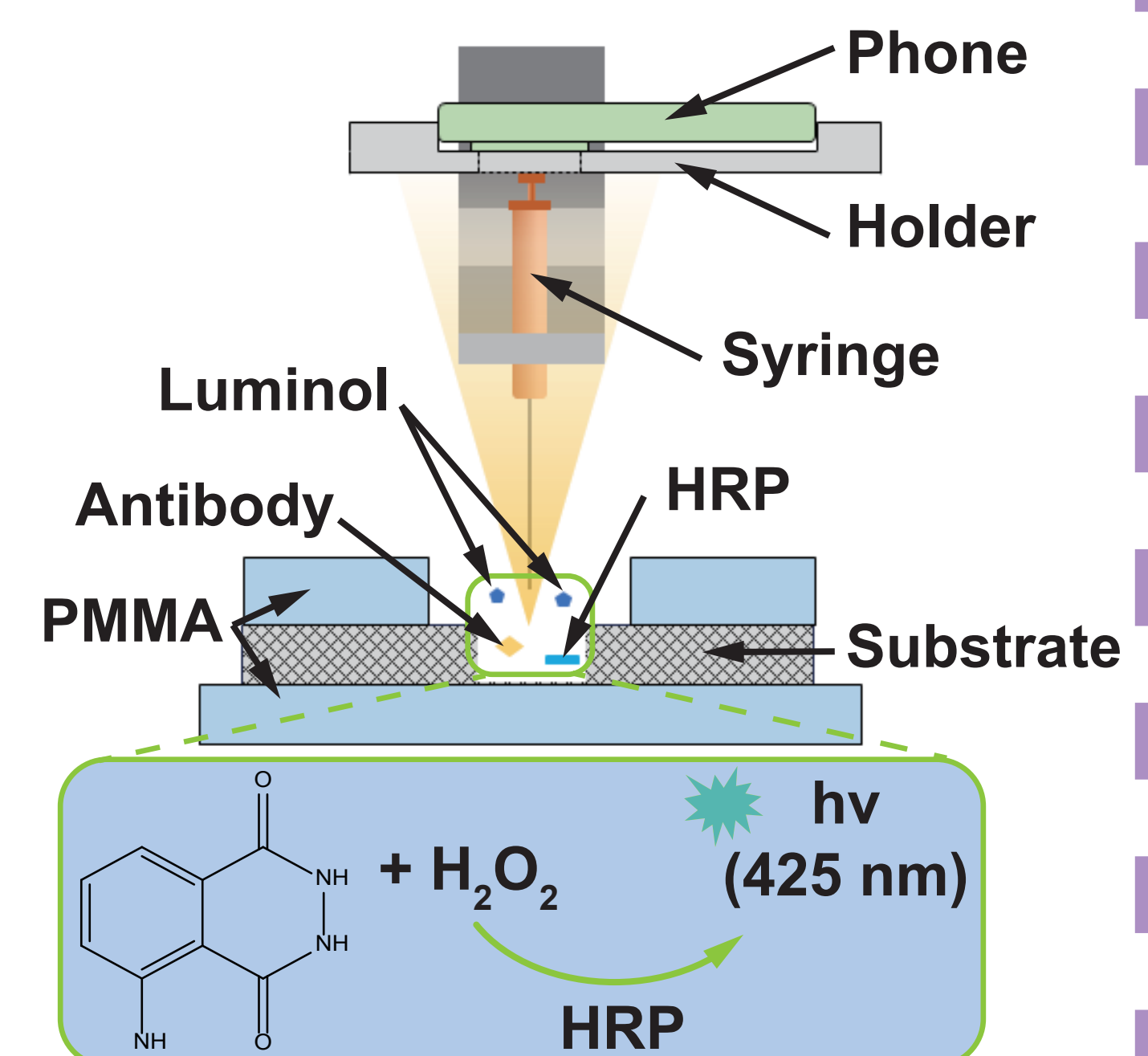


Fig. 2. Cross sectional view of μ PAD.

- The rotary valve on the μ PAD controls the on/off state of microchannels, achieving the connection of various regions (Fig. 3).

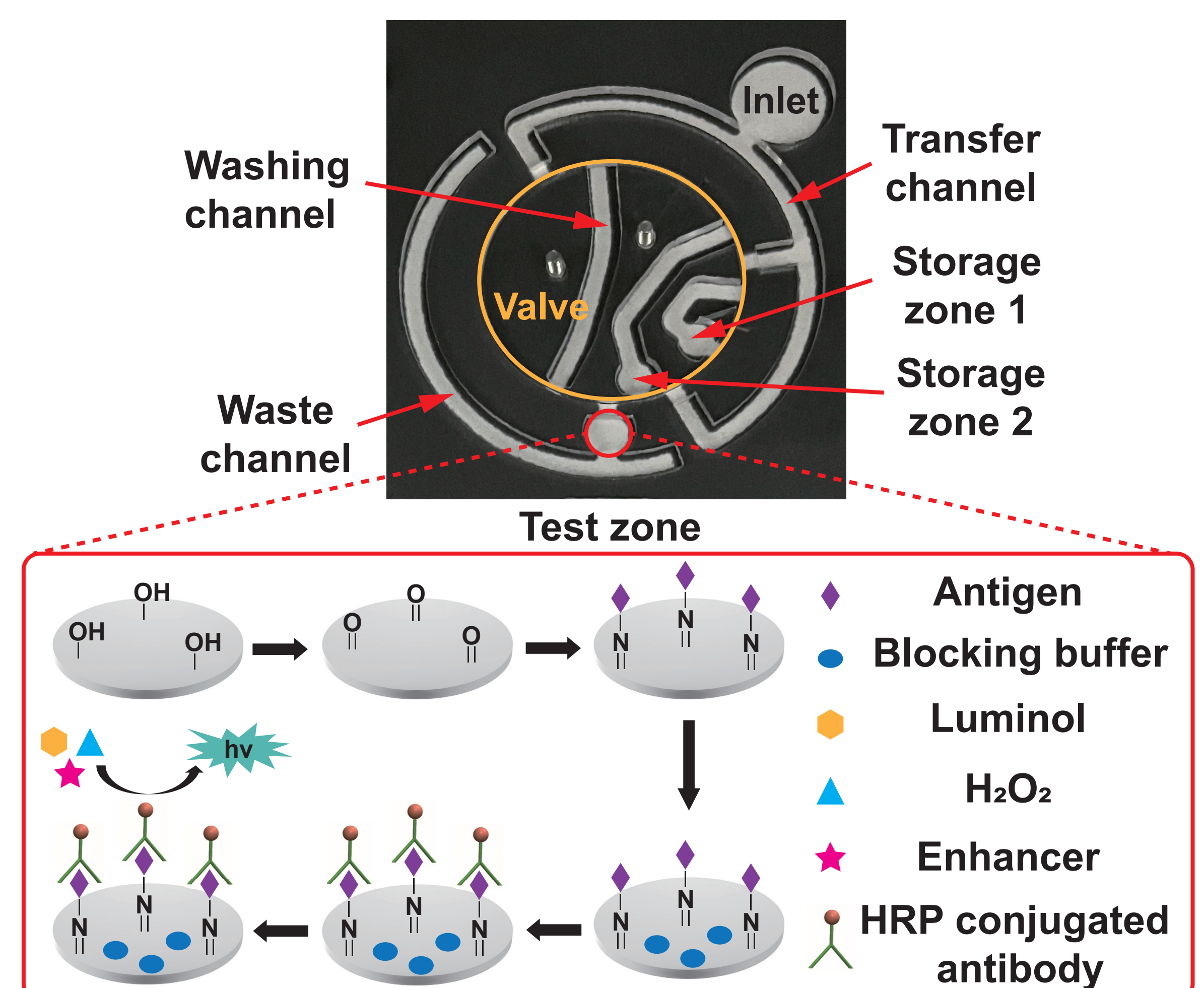


Fig. 3. The photo of developed μ PAD consisted of a rotary valve and a surrounding chip with the protocol of CL ELISA in the test zone.



Ruiqi Yong

Undergraduate Student (Year 3)
Xi'an Jiaotong-Liverpool University
Email: ruiqi.yong1118@gmail.com
Web: <https://ruiqiyong.github.io/>



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