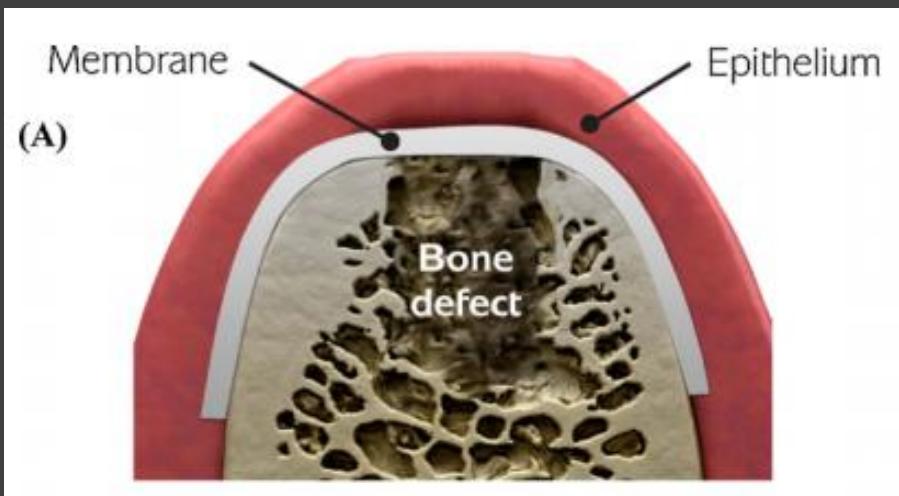
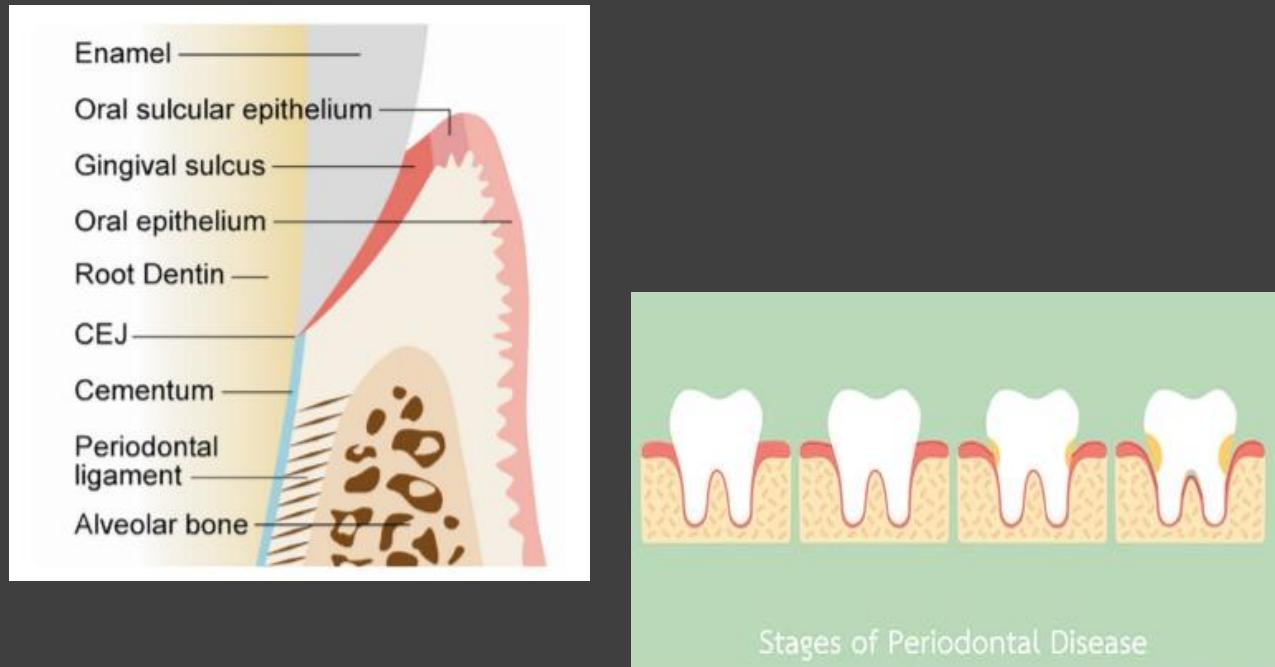


3D-Bioprinted PCL/GelMA-HA Scaffolds for Guided Bone Regeneration (GBR)

Ryan Roessler

University of Alabama at
Birmingham

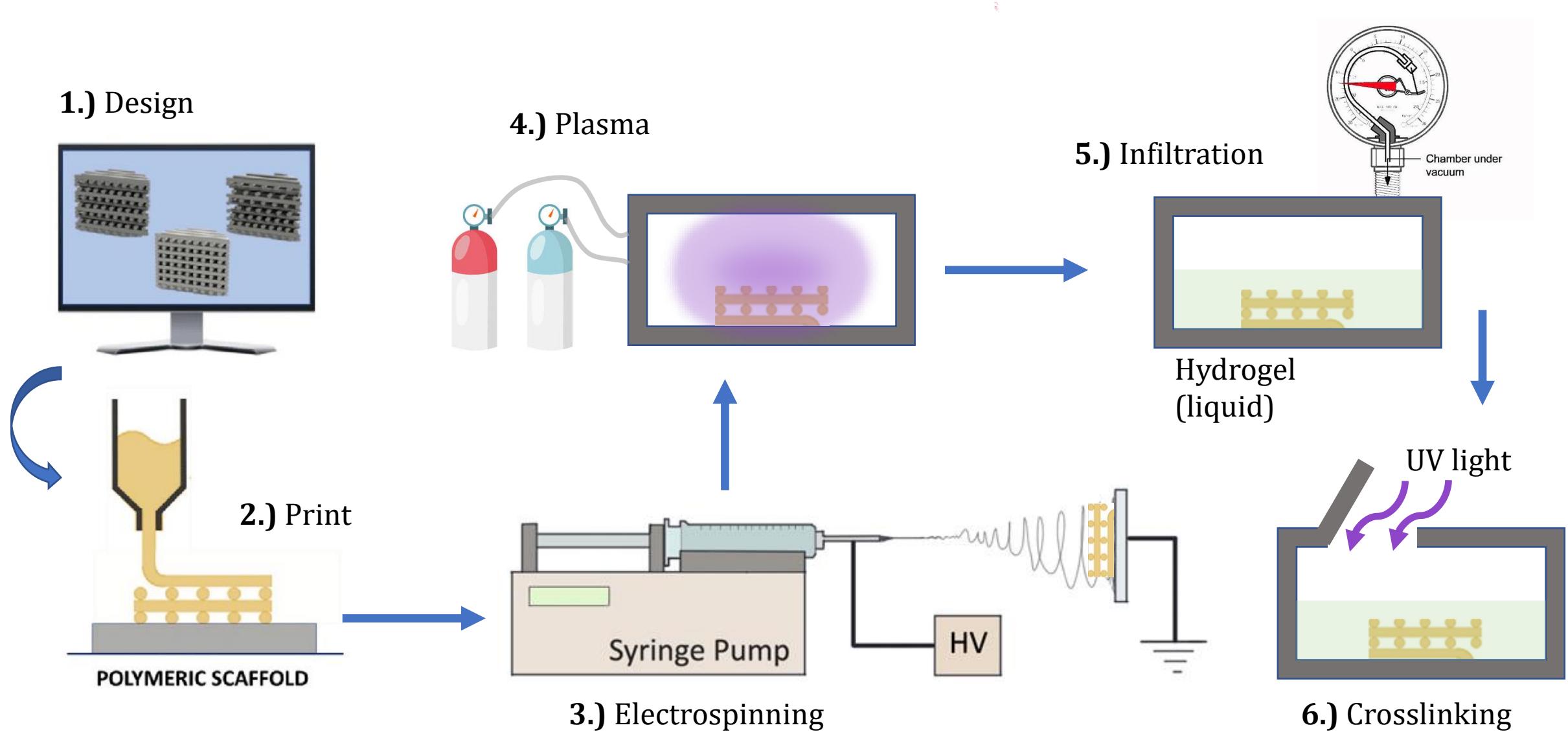




Periodontitis

- Inflammatory gum disease, erodes gums and enamel
- Objective: Synthesize a membrane to fill space and regenerate tissue
 - Must be biocompatible, biodegradable and bioactive material
- Marco C. Bottino, Vinoy Thomas, Gudrun Schmidt, Yogesh K. Vohra, Tien-Min Gabriel Chu, Michael J. Kowollik, Gregg M. Janowski, 'Recent advances in the development of GTR/GBR membranes for periodontal regeneration—A materials perspective', *Dental Materials*, vol 28, Issue 7, 2012, pp 703-721. <https://doi.org/10.1016/j.dental.2011-2.04.022>.
- <https://www.shutterstock.com/search/gum+disease+cartoon>

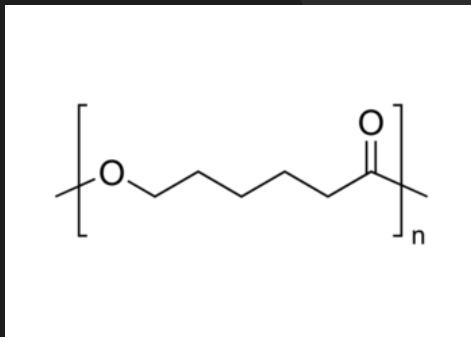
Graphical Abstract



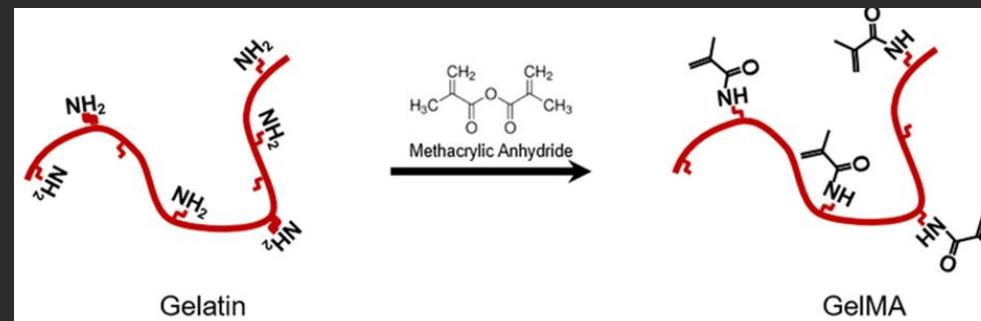
Materials

Polycaprolactone (PCL)

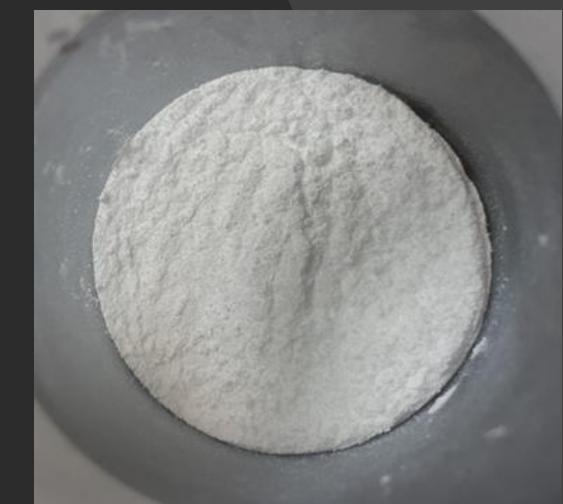
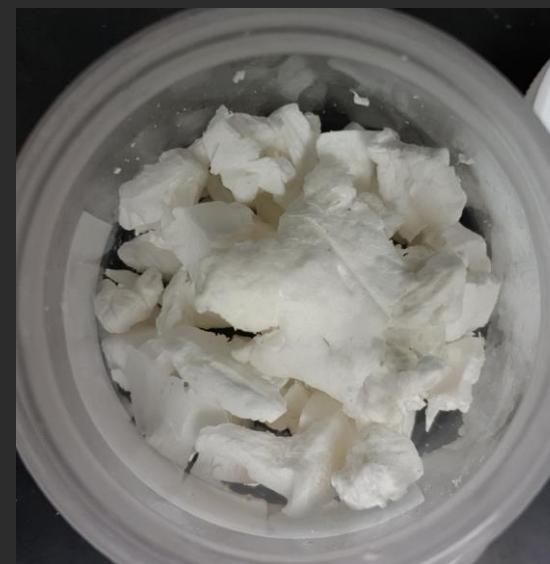
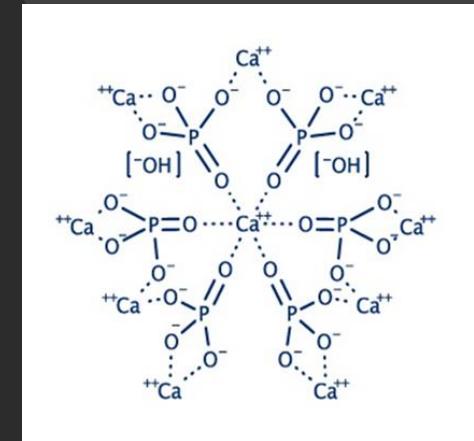
- Visco-elastic polyester
- FDA approved & biocompatible
- Slow degradation rate



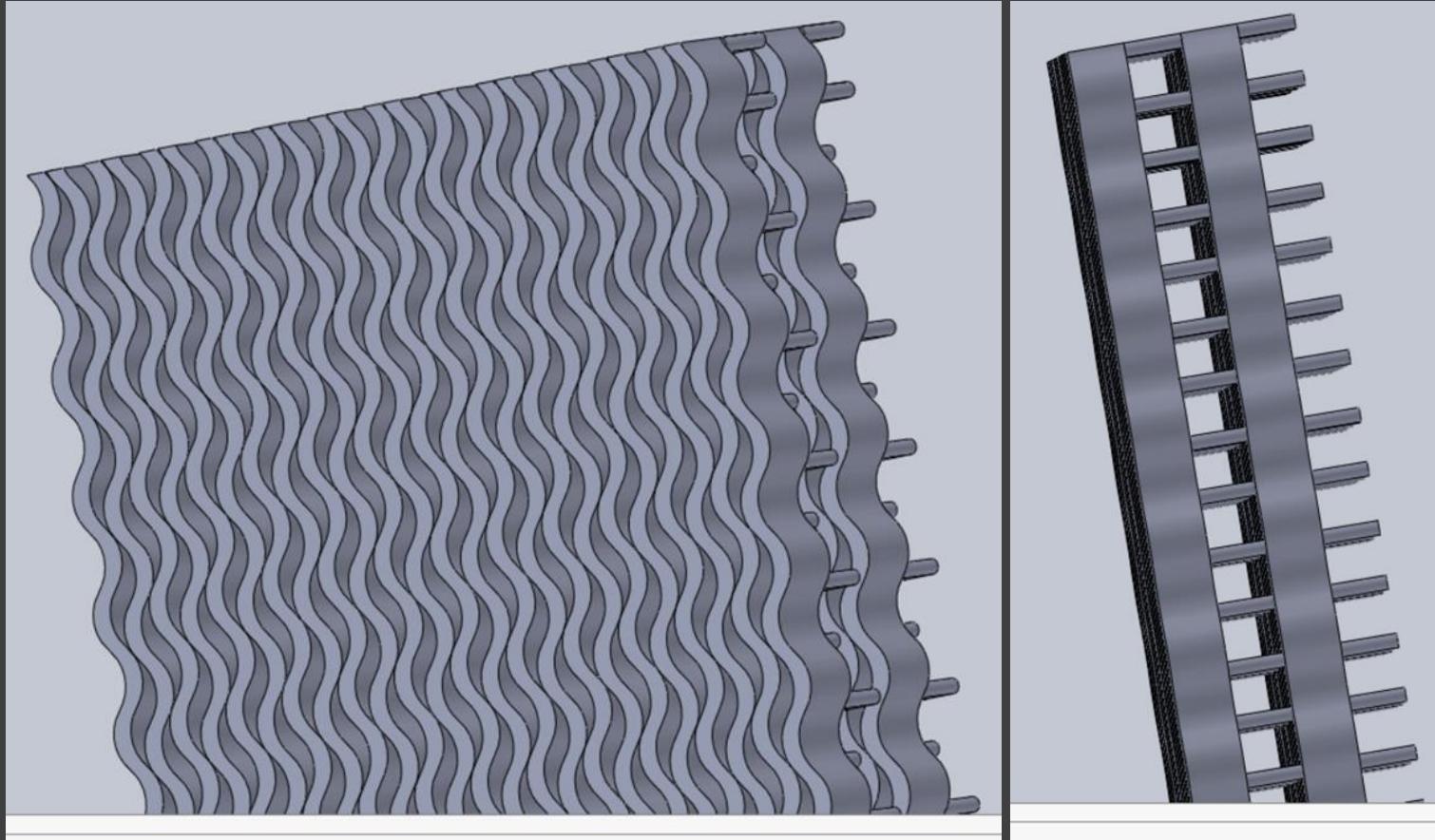
Gelatin methacryloyl (GelMA)



Hydroxyapatite (HA)



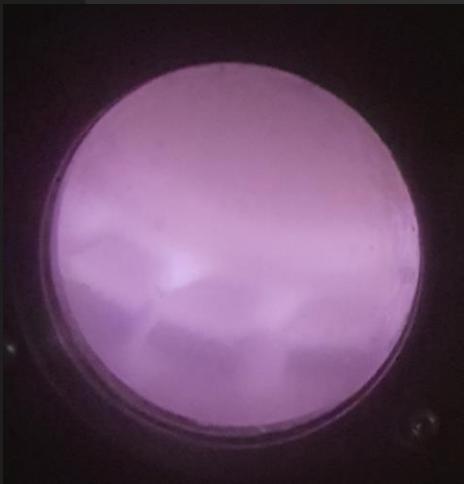
Scaffold Design: SolidWorks CAD Software



- Favorite design; couldn't print due to resolution limitations

Plasma Modification

- Provides surface-level functional groups for improved interfacing with GelMA
- Low-Temperature Plasma (LTP) treatment
 - Non-equilibrium
 - Low-pressure
- 45 W radio frequency (RF), 15sccm, ~500mTorr



Nitrogen (N₂)



Oxygen (O₂)



Hydrogen (H₂)



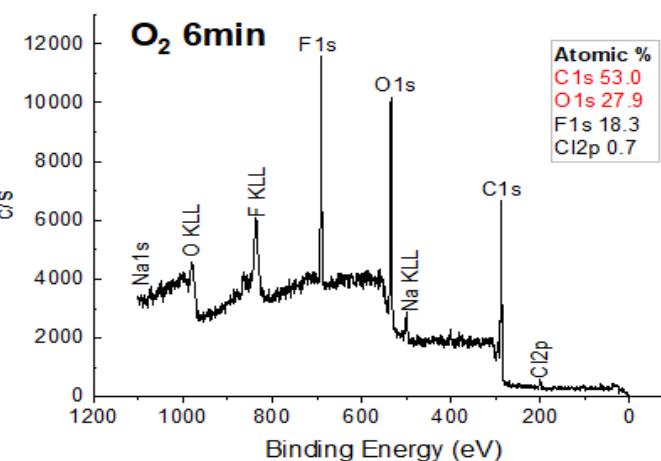
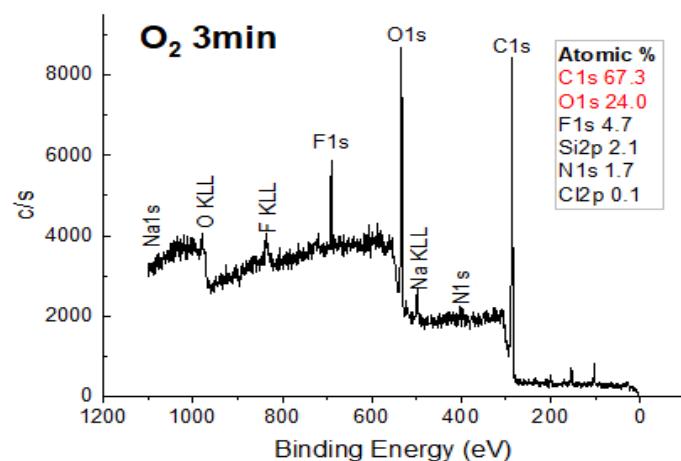
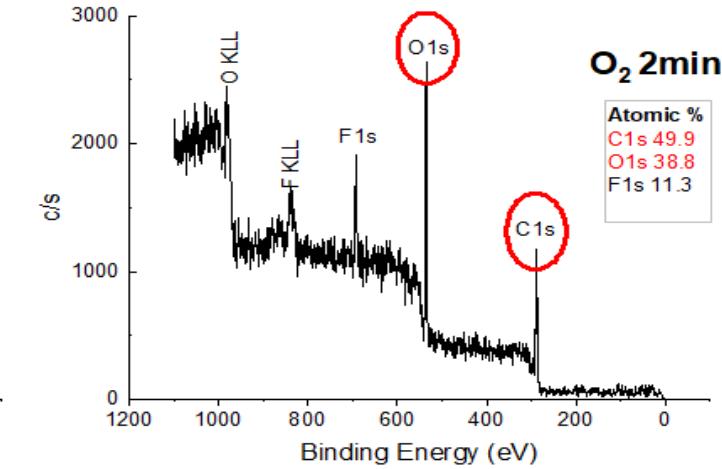
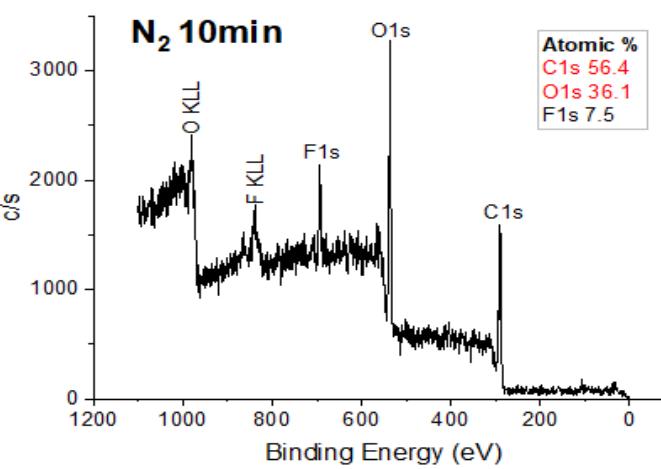
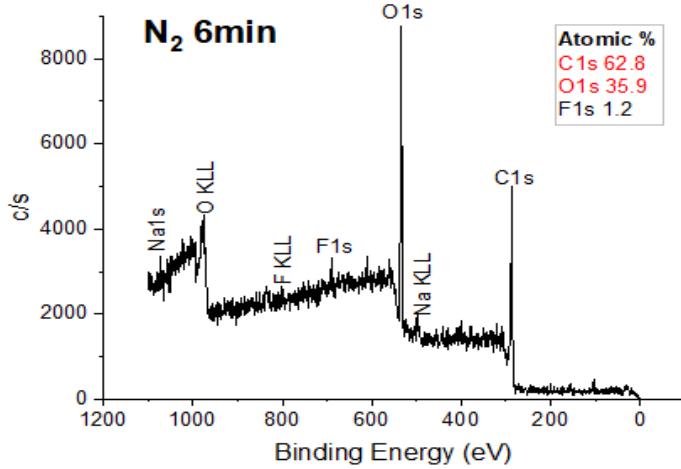
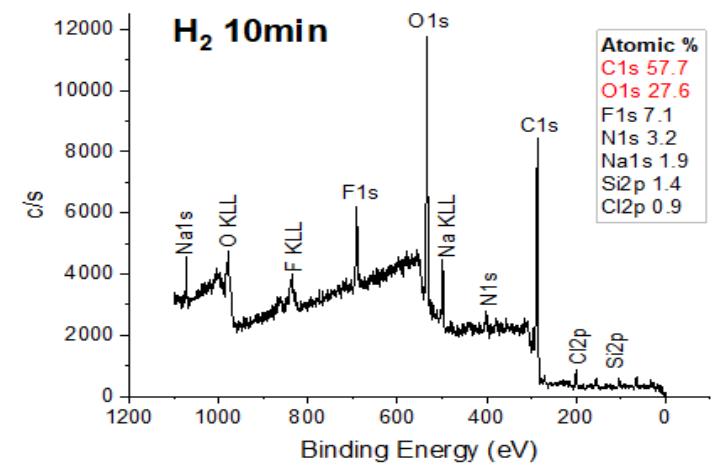
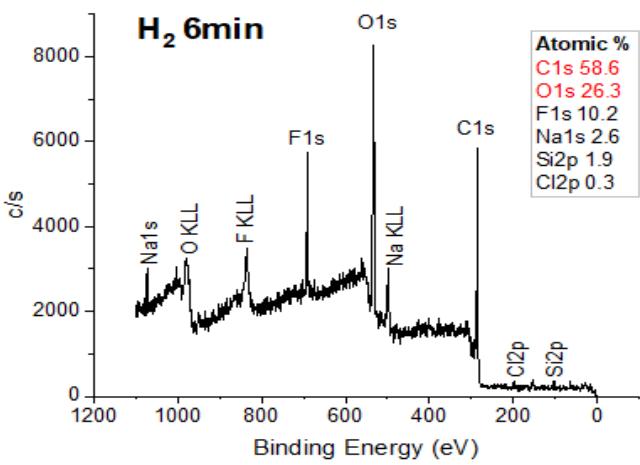
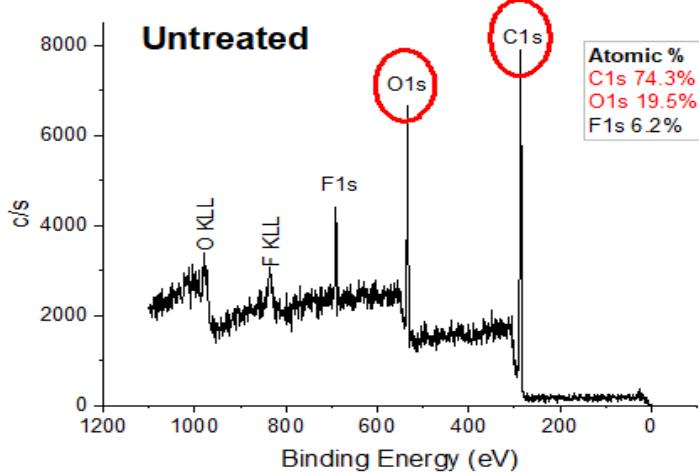
Water Contact Angle (Hydrophilicity)

Time after drop:	1s	10s	30s
Plasma		Contact Angle (°)	
Untreated	80.8 ± 2.0	77.9 ± 2.0	72.2 ± 2.0
N 10s	27.8 ± 2.0	0	0
N 20s	0	0	0
N 30s	0	0	0
O 10s	0	0	0
O 20s	0	0	0
O 30s	0	0	0
H 10s	82.2 ± 2.0	78.2 ± 2.0	76.1 ± 2.0
H 20s	0	0	0
H 30s	N/A	N/A	52.8 ± 2.0

X-Ray Photoelectron Spectroscopy (XPS)

Oxygen treatment for 6+ minutes began to noticeably etch the surface

Plasma Treatment	Surface Element	Relative Percentage (%)
None (Control)	C	74.3
	O	19.5
Nitrogen 6min	C	62.8
	O	35.9
Nitrogen 10min	C	56.4
	O	36.1
Oxygen 2min	C	49.9
	O	38.8
Oxygen 3min	C	67.3
	O	24
	N	1.7
Oxygen 6min	C	53
	O	27.9
	O	26.3
Hydrogen 6min	C	58.6
	O	26.3
Hydrogen 10min	C	57.7
	O	27.6
	N	3.2



Fabrication/Optimization of Hydrogel

- GelMA and Irgacure 2959 (photoinitiator) were separately mixed in dPBS
- Irgacure was added to GelMA mixture in varying concentrations
- Mixture was photopolymerized with UV light (365nm) for different amounts of time
- Optimal combination was 1.5% photoinitiator, crosslinked for 3 minutes
- For GelMA-HA, nano hydroxyapatite (HA) powder was added at a 5% w/v concentration



Optimization of Hydrogels via Rheology

3-minute crosslink

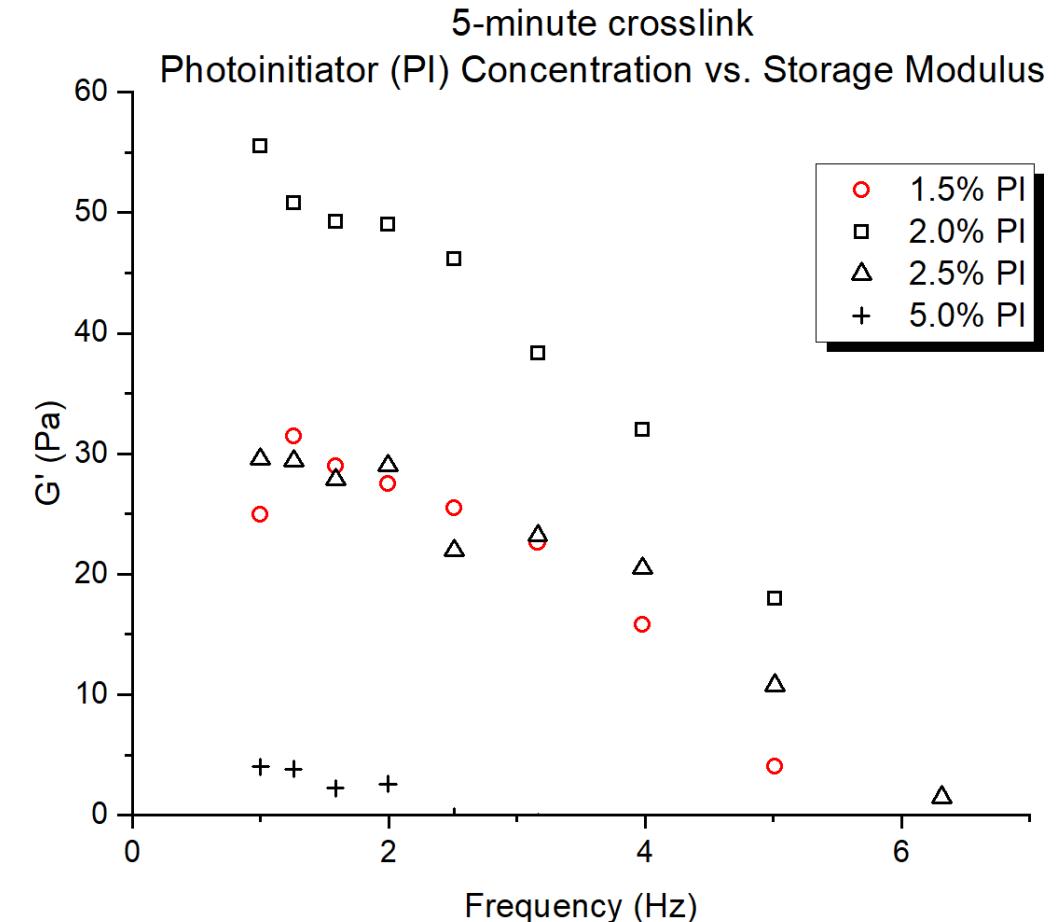
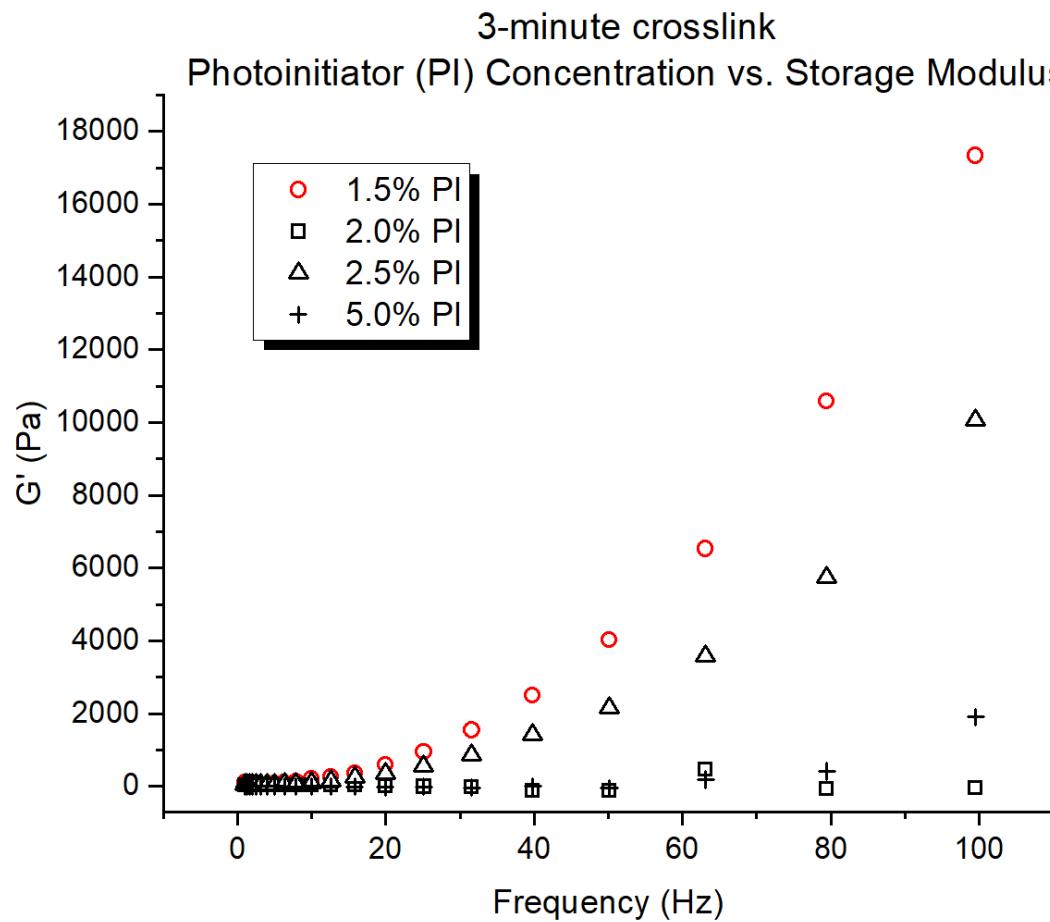
PI (% w/v)	Max G' (Pa)
1.50%	17340
2.00%	464.5
2.50%	10070
5.00%	1908

5-minute crosslink

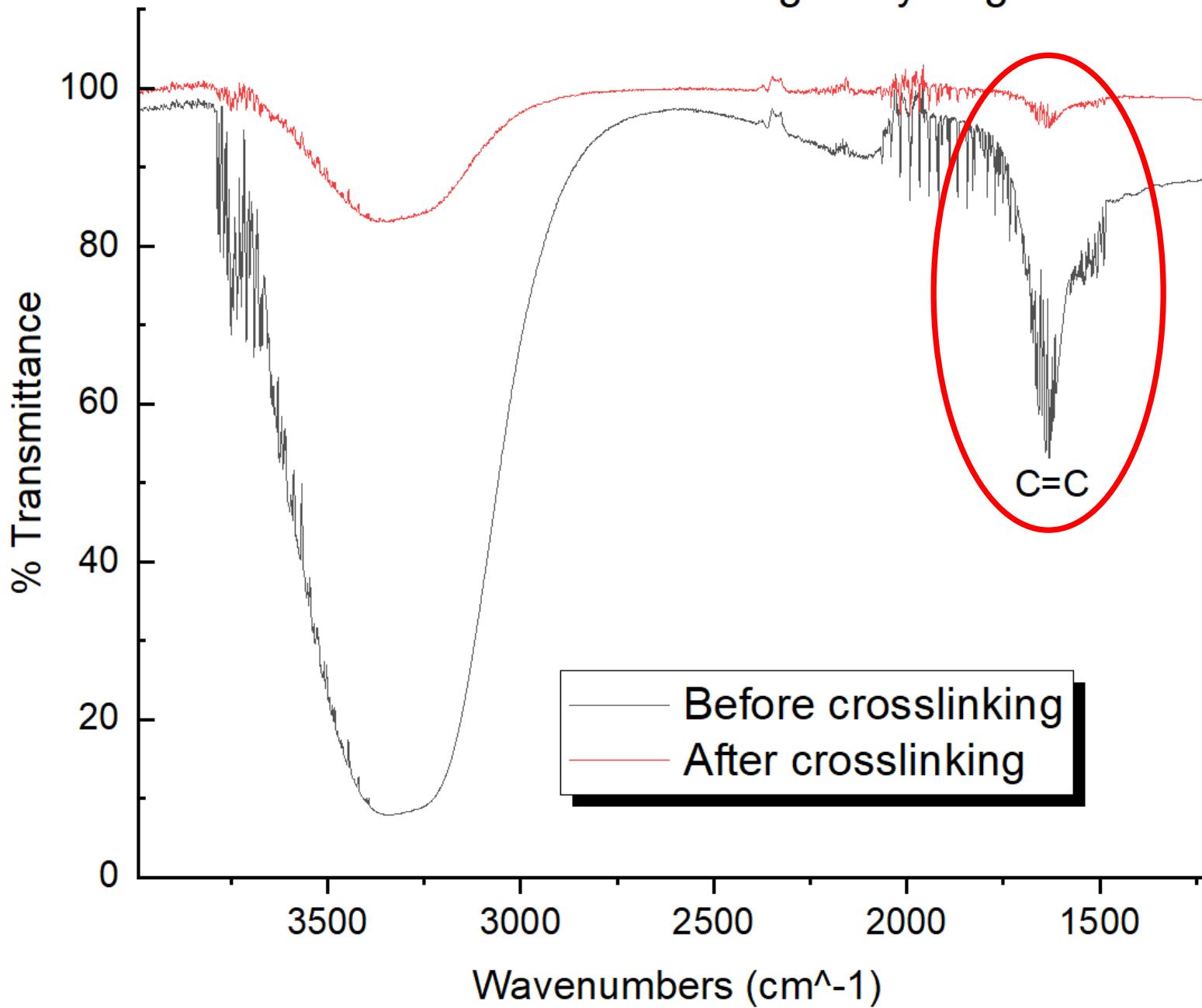
PI (% w/v)	Max G' (Pa)
1.50%	31.46
2.00%	55.53
2.50%	29.58
5.00%	4.014



Storage Modulus



Evidence of Crosslinking in Hydrogel



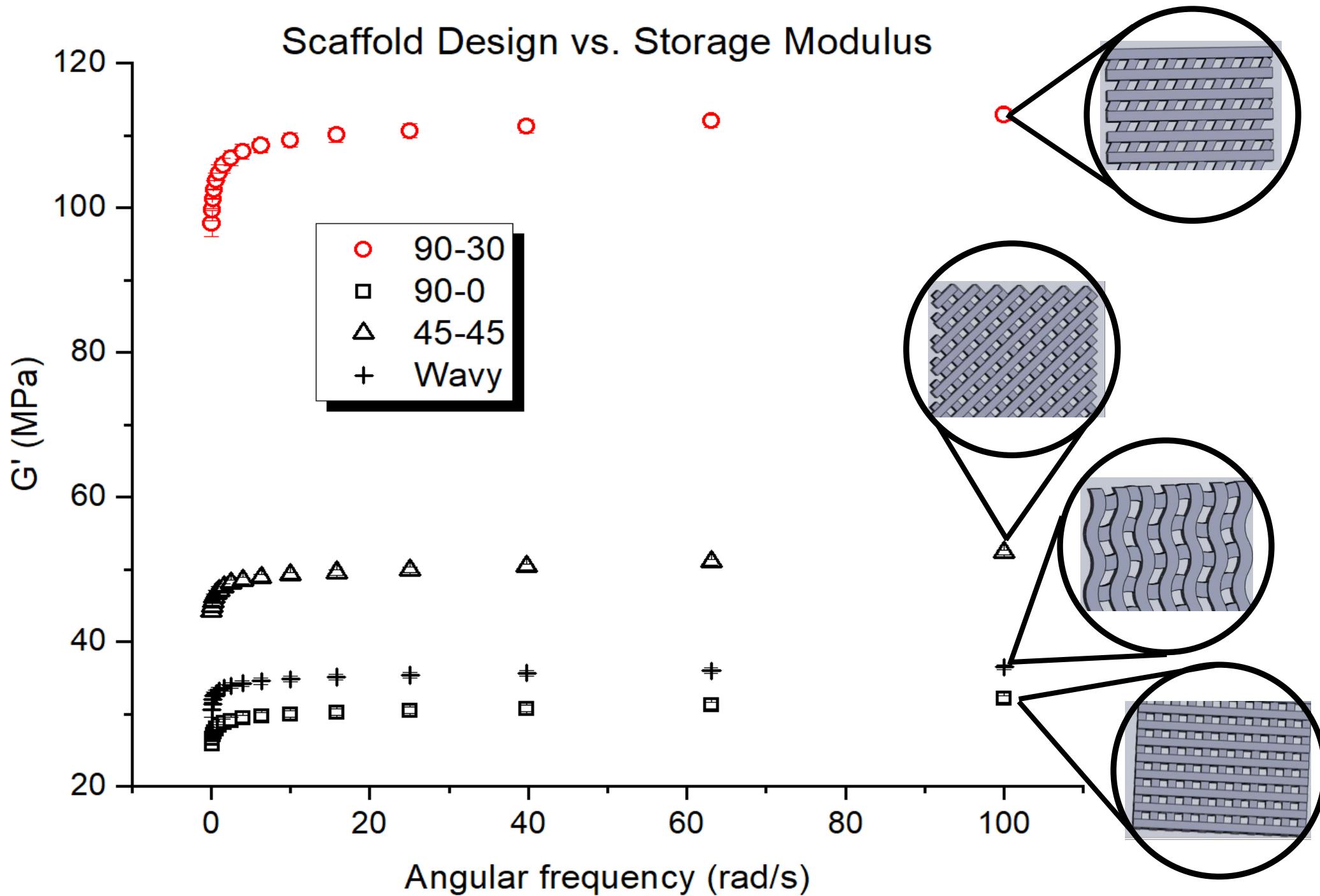
Hydrogel Infiltration

- White is GelMA-HA composite
- Poured GelMA/GelMA-HA solution over scaffold
- De-gassed in a vacuum chamber for infiltration into pores
- Crosslinked with 365nm UV light
- Removed scaffolds with tweezers

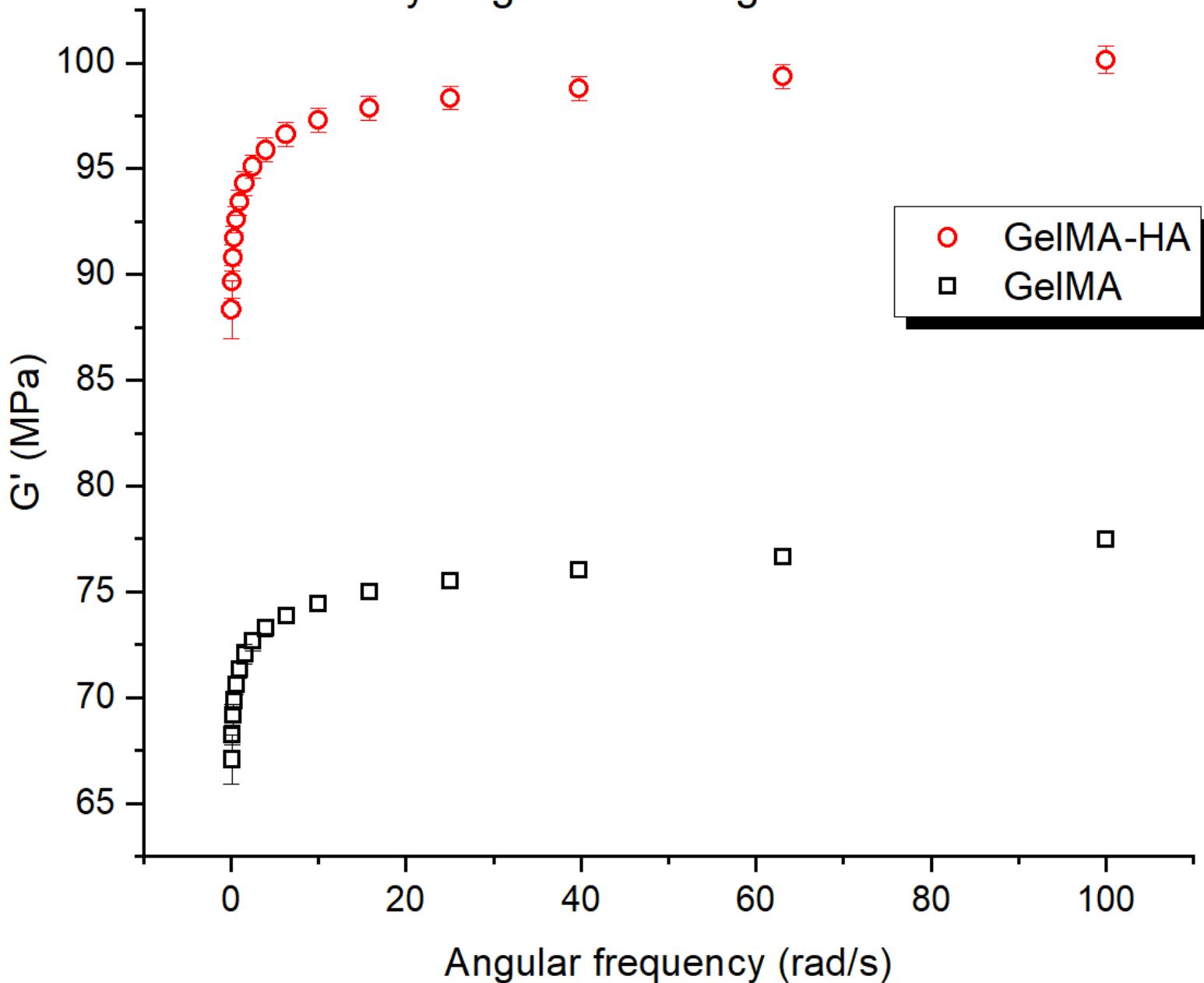


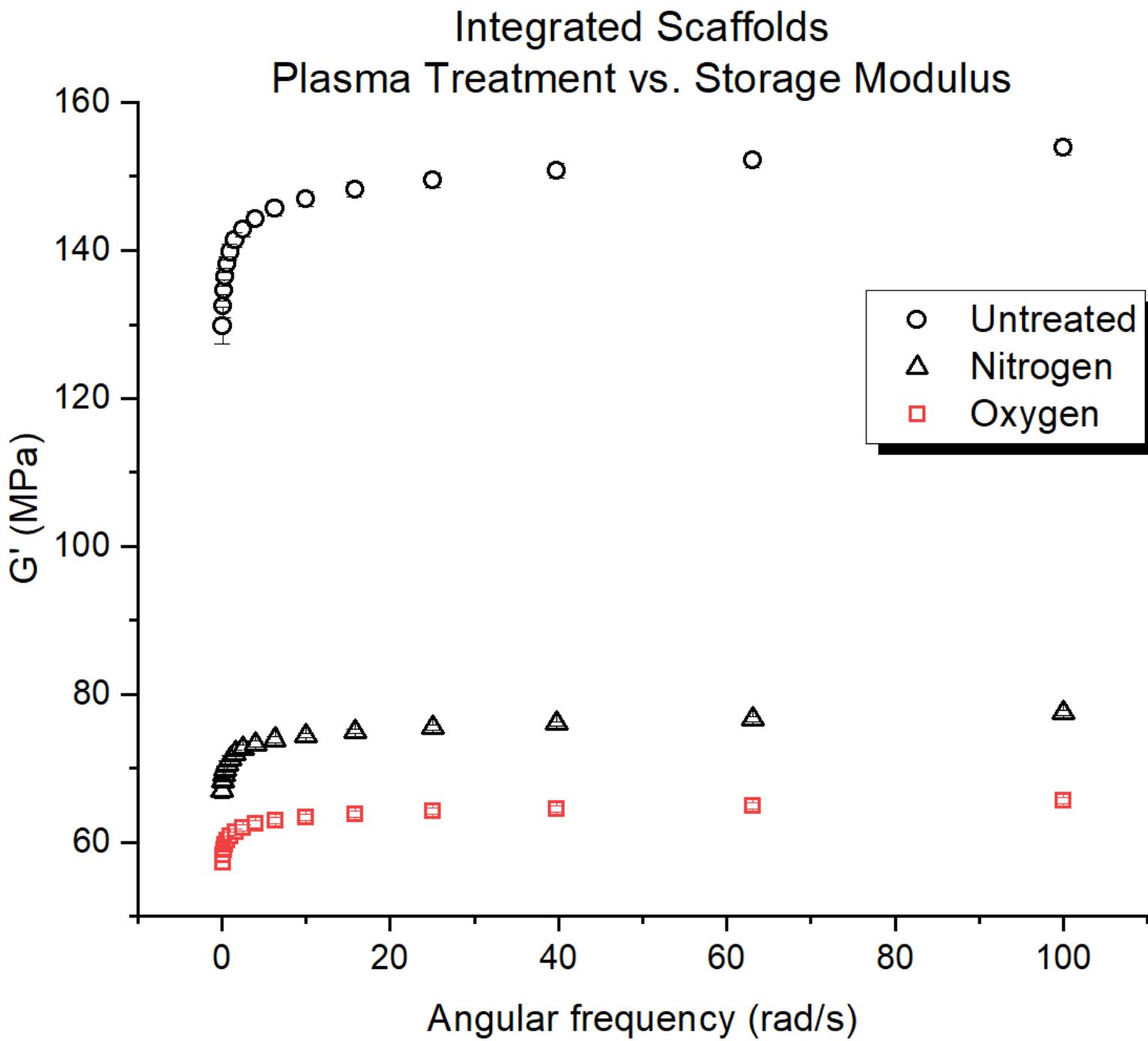
Mechanical Strength Testing (Torsion)





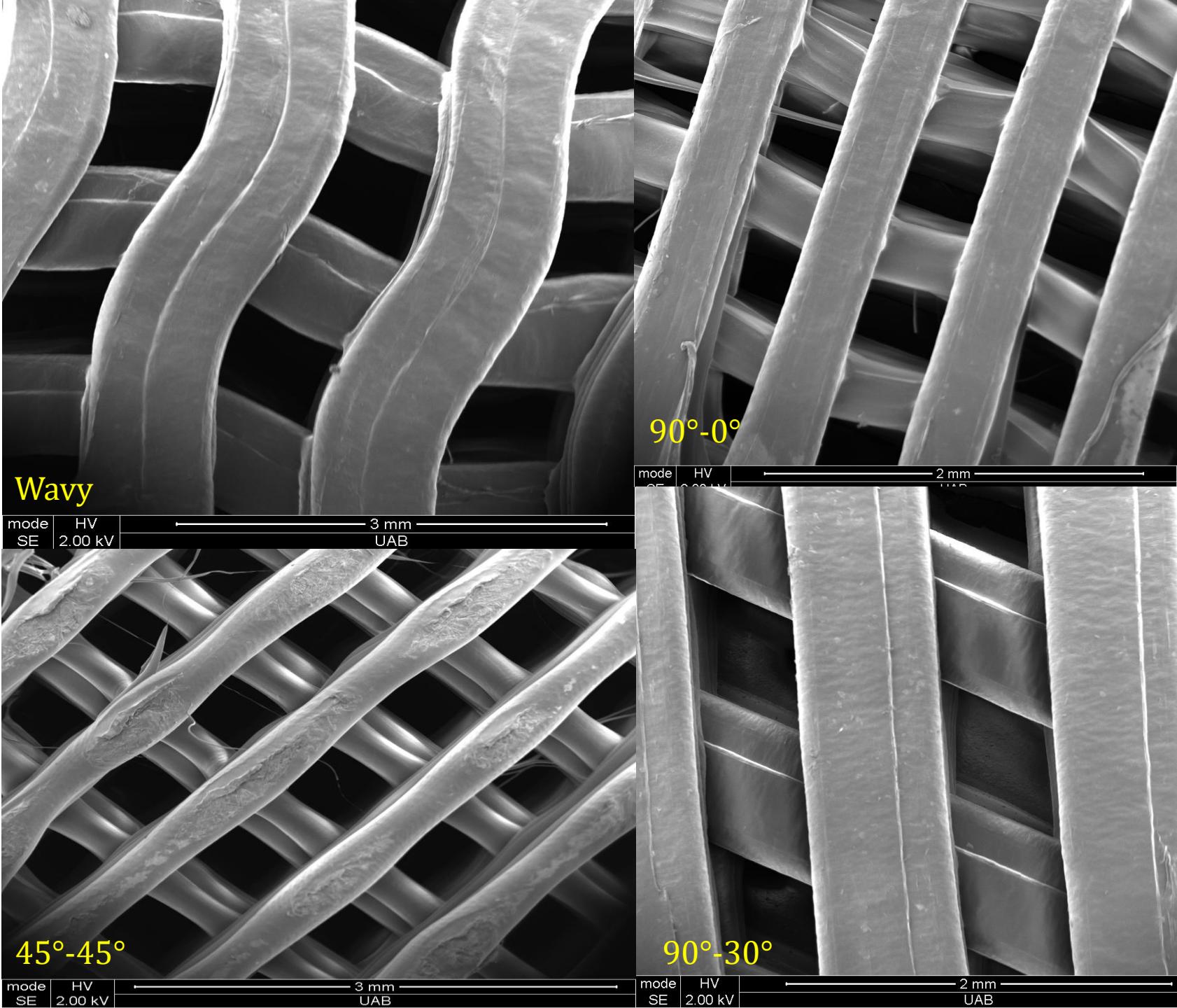
Infiltrated Scaffolds Hydrogel vs. Storage Modulus

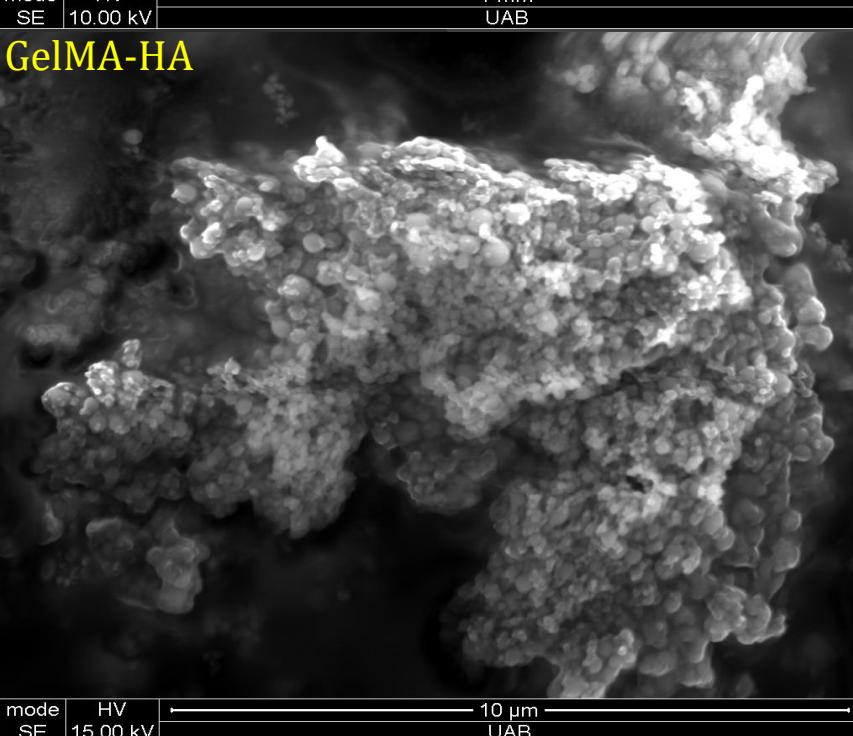
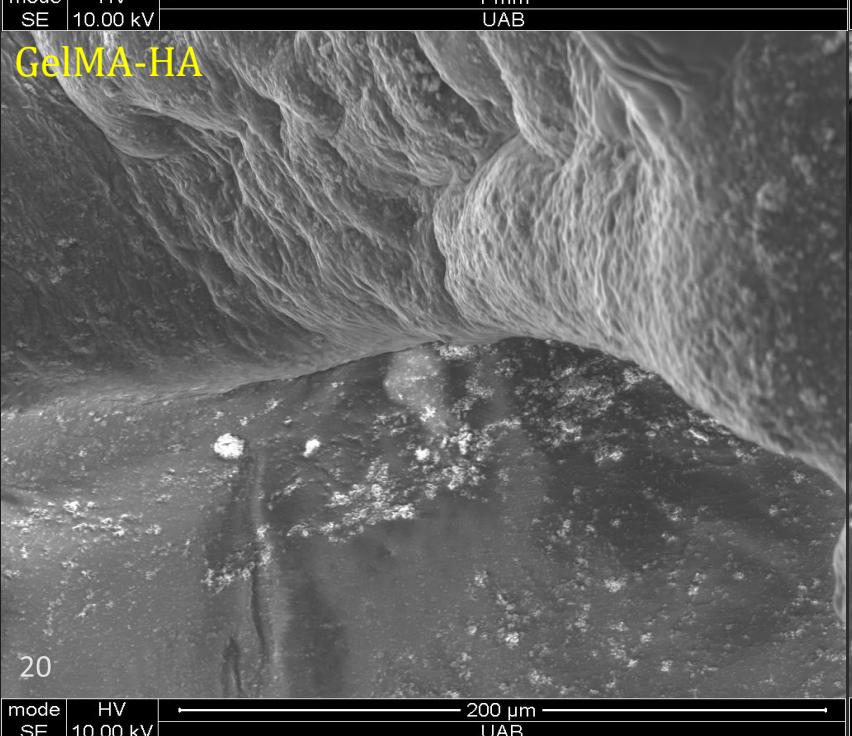
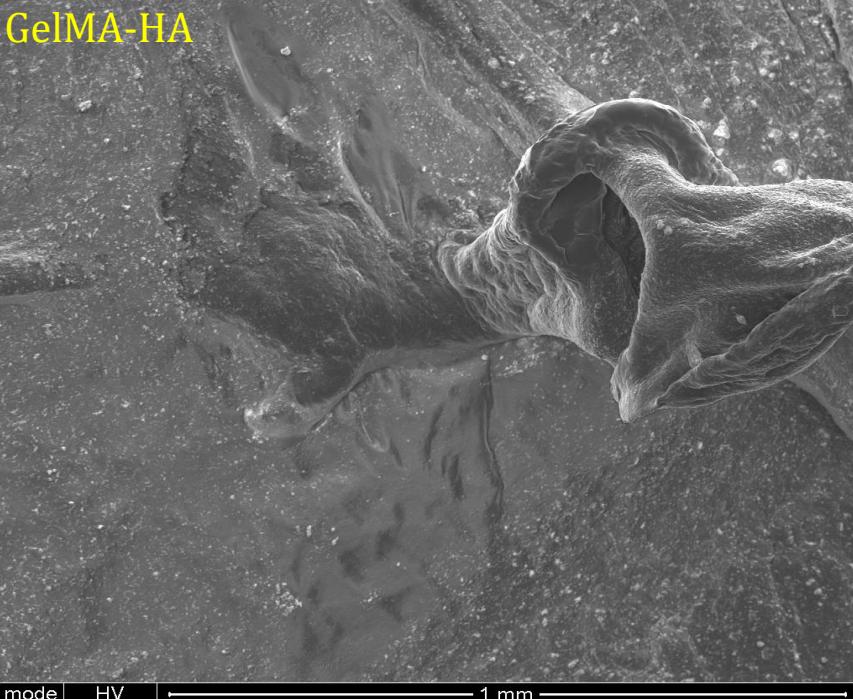
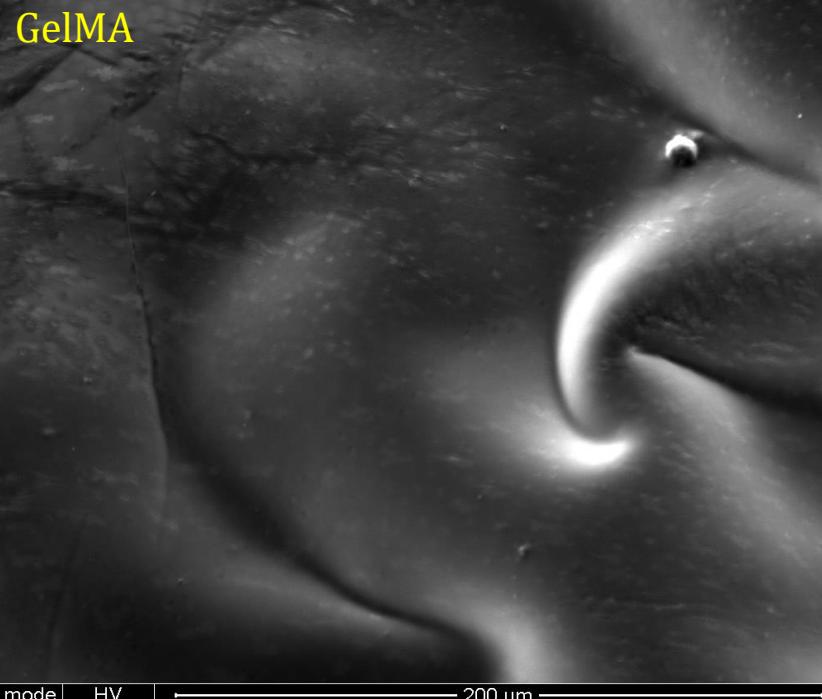
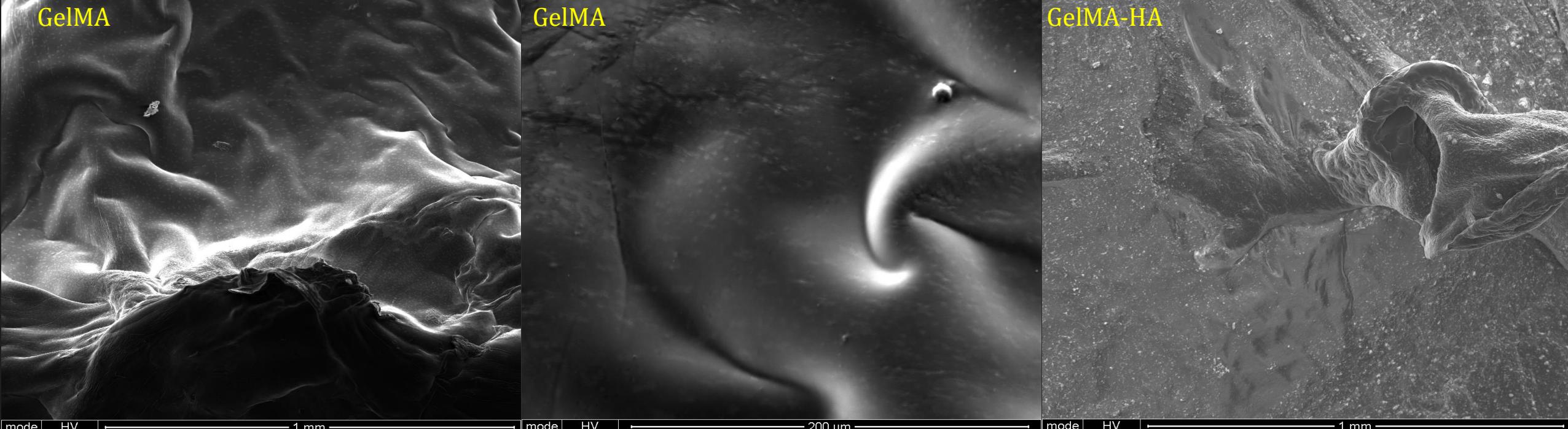




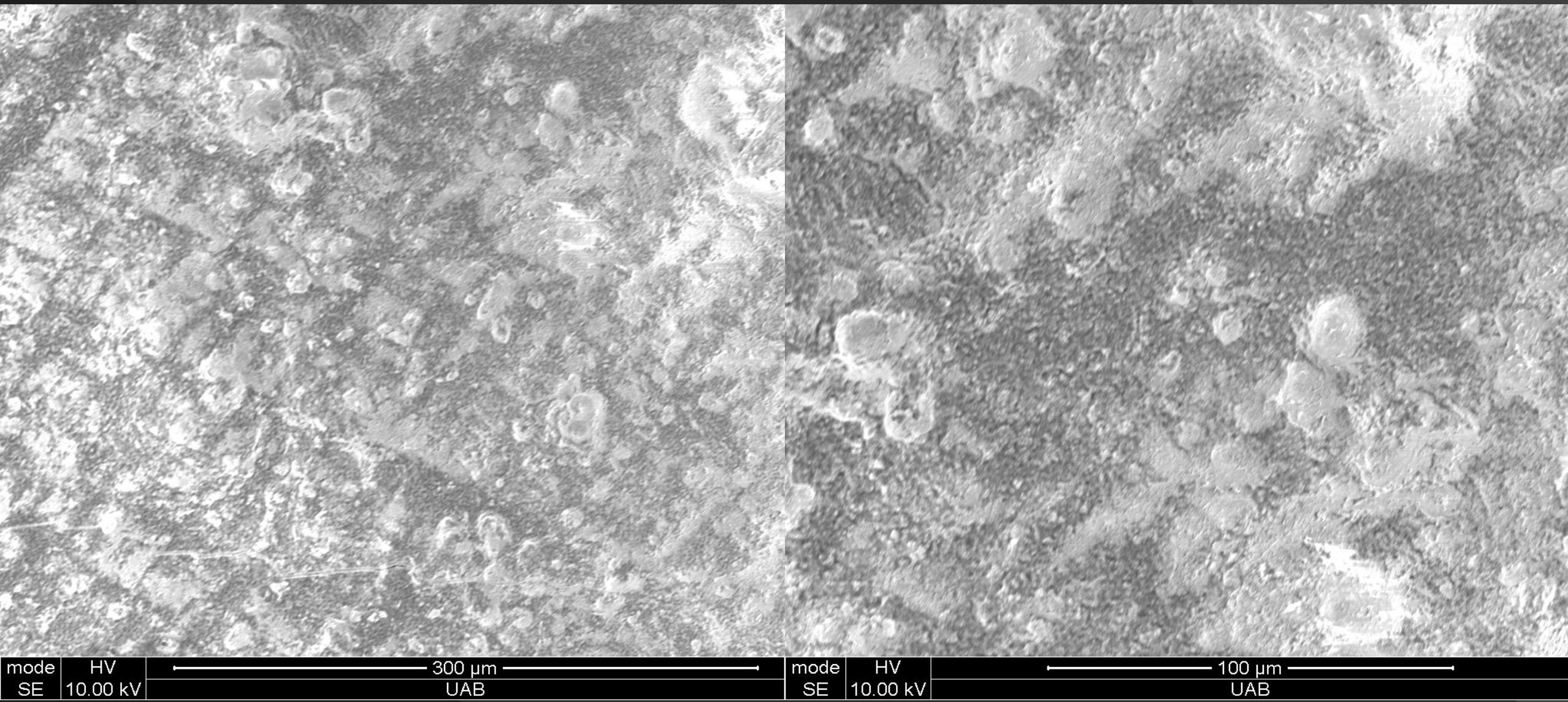
Scanning Electron Microscopy (SEM)

Scaffolds of varying designs
and pore structure

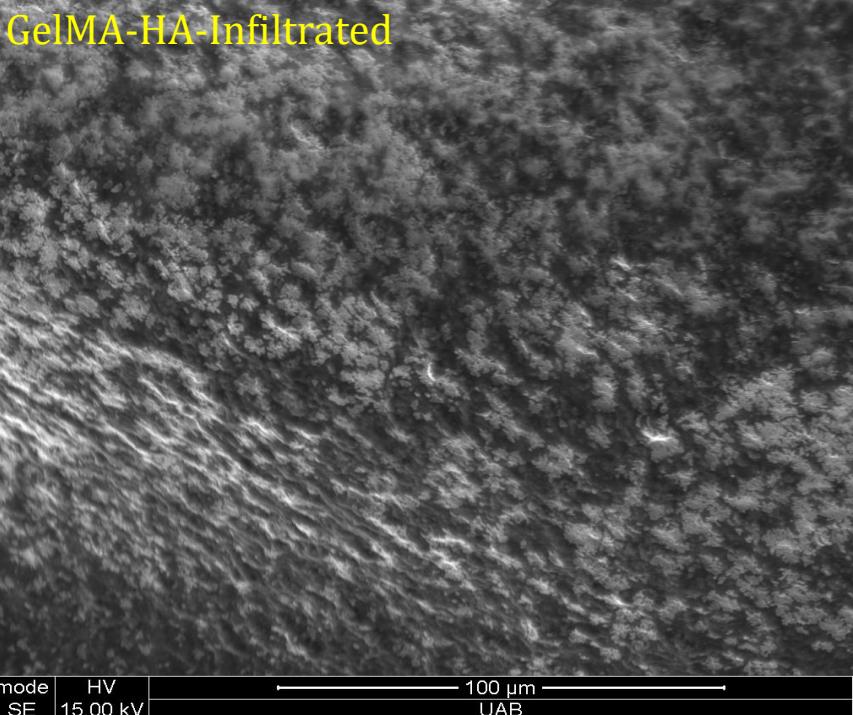
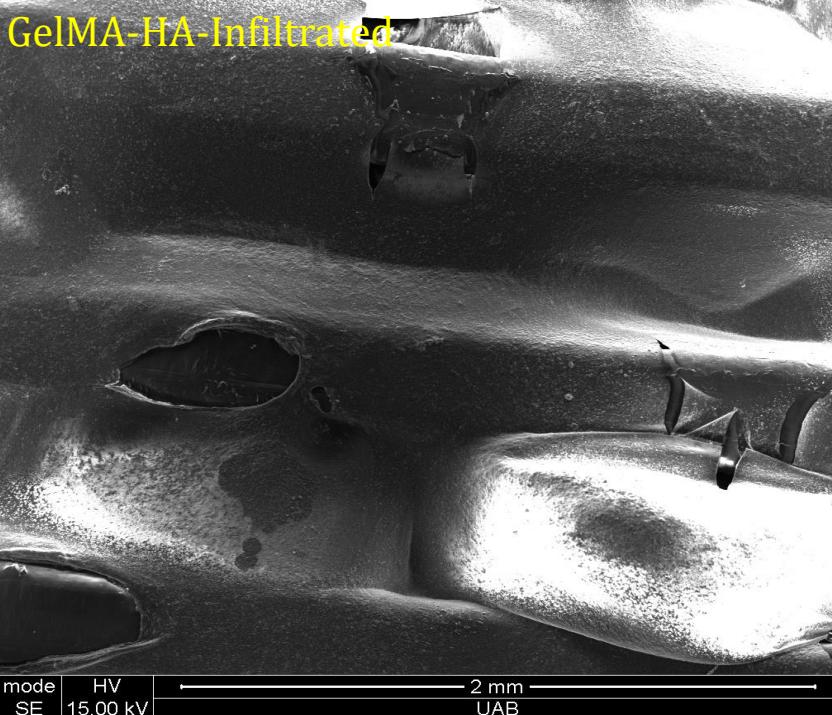
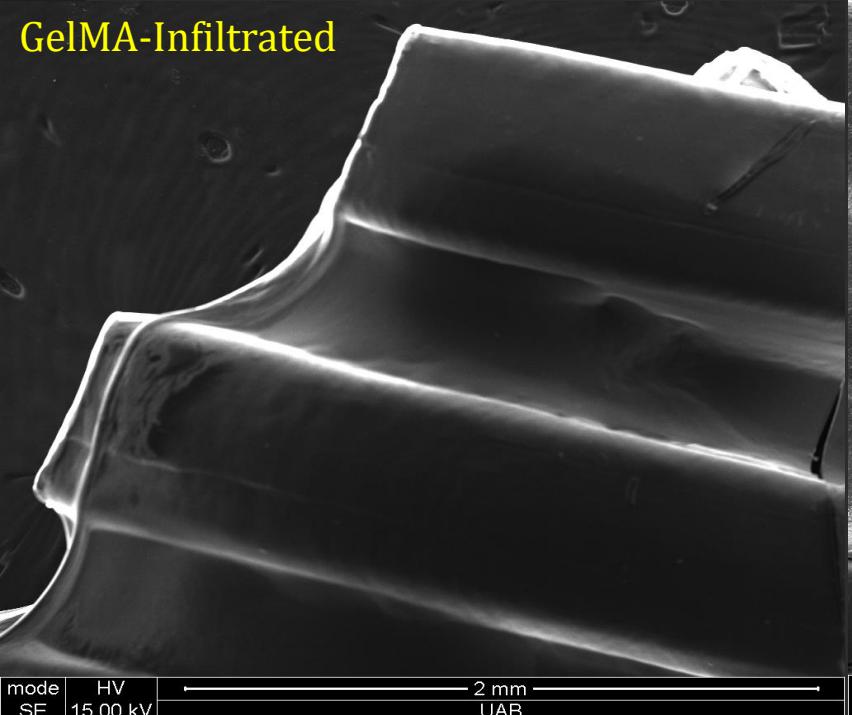




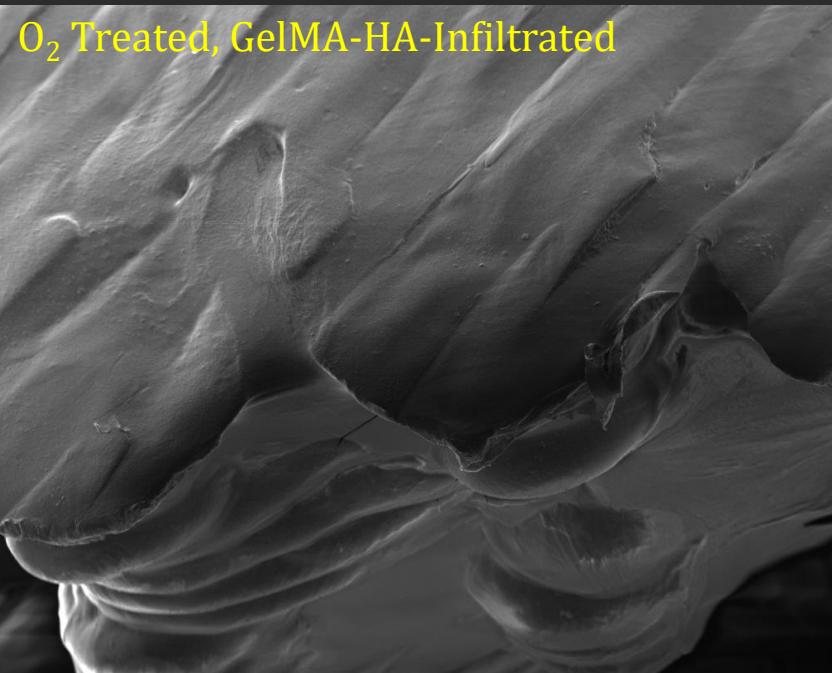
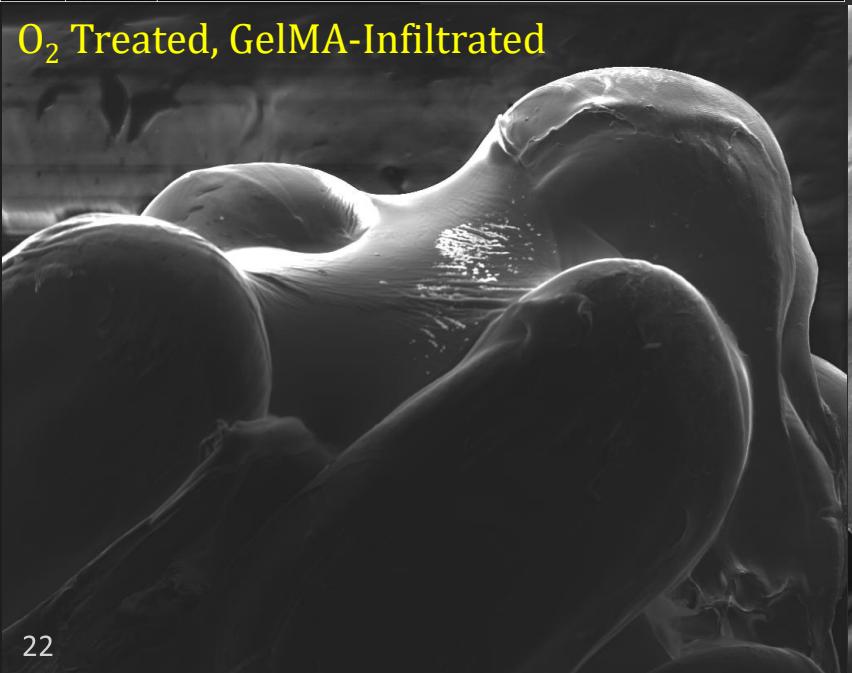
Hydroxyapatite



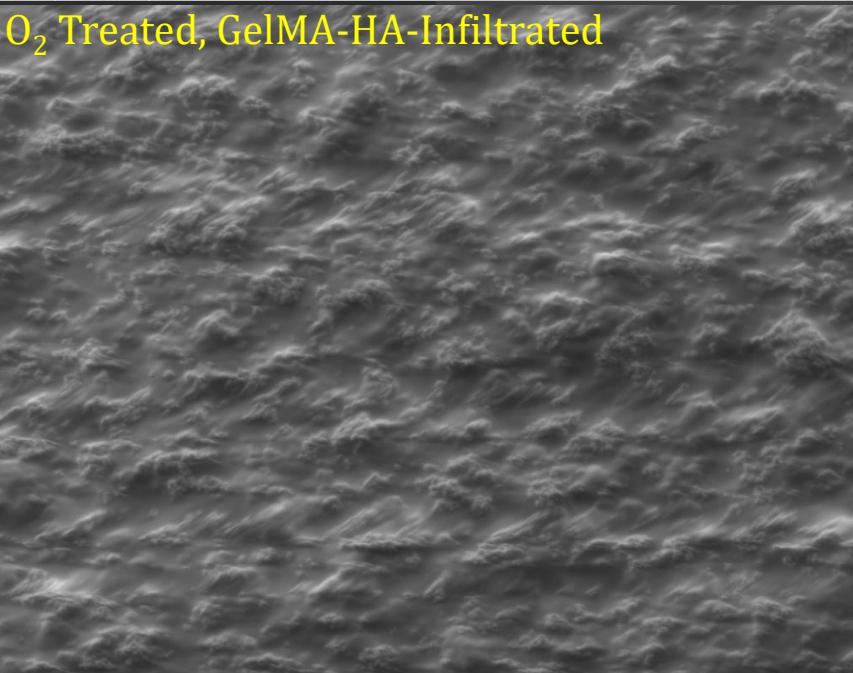
GelMA-Infiltrated



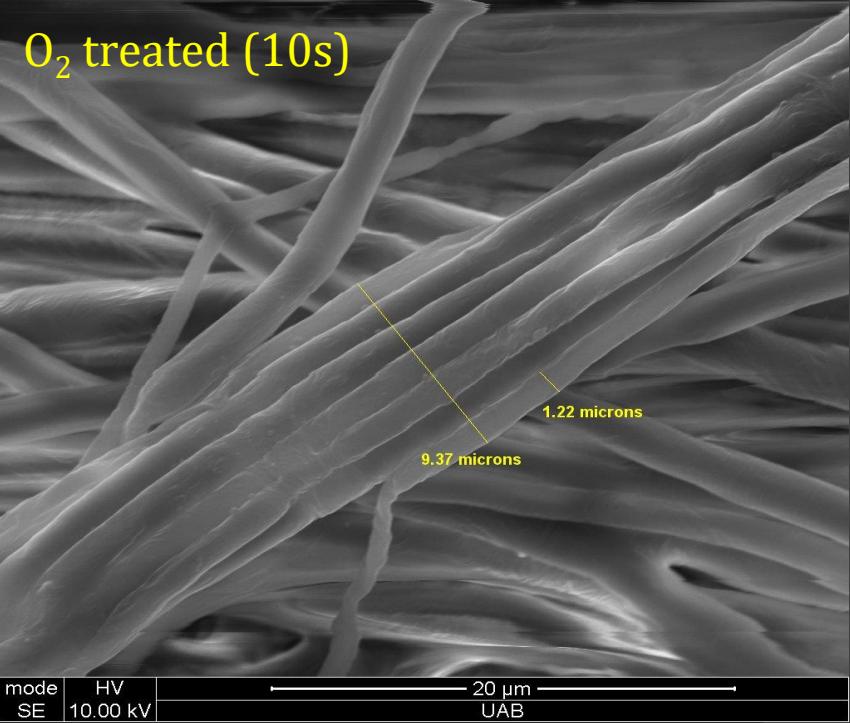
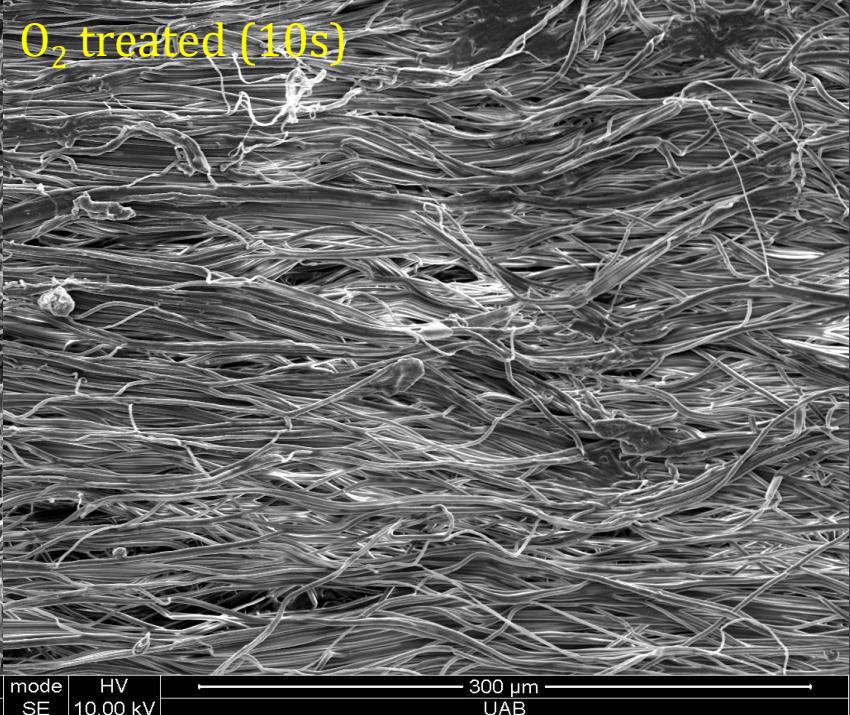
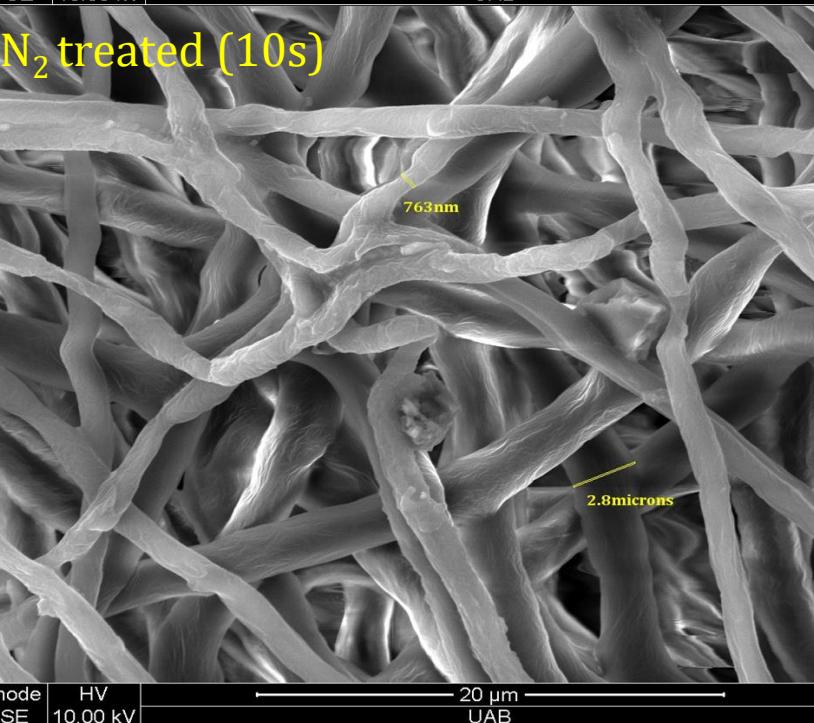
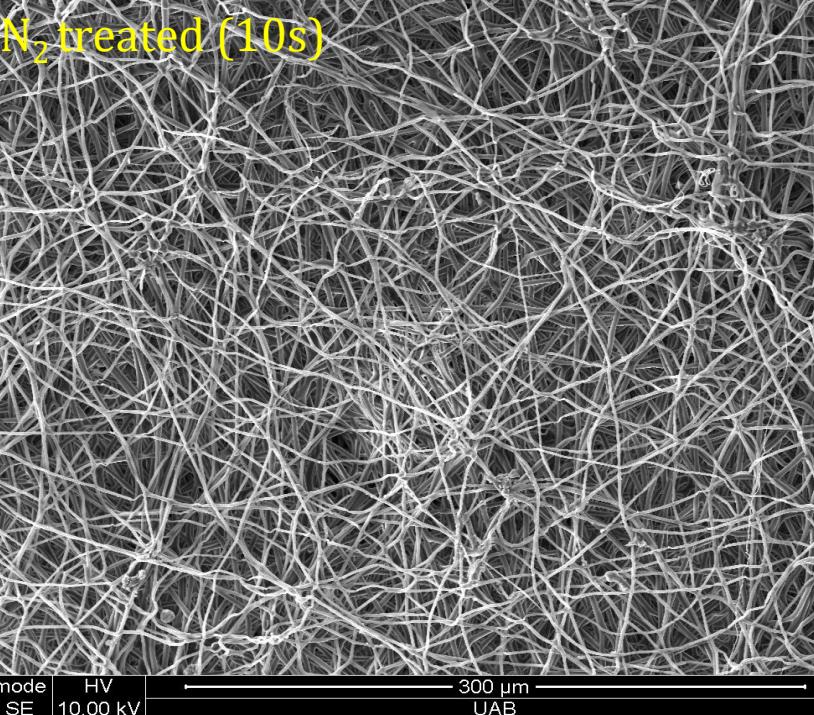
O₂ Treated, GelMA-Infiltrated

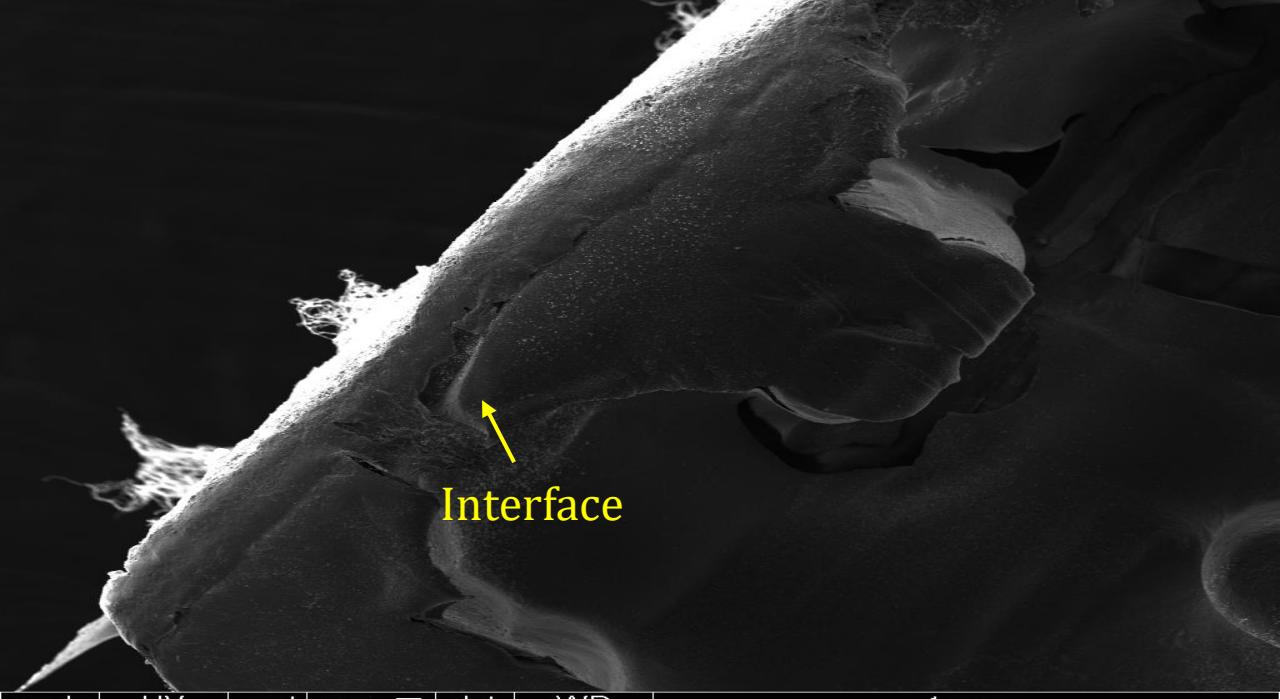


O₂ Treated, GelMA-HA-Infiltrated

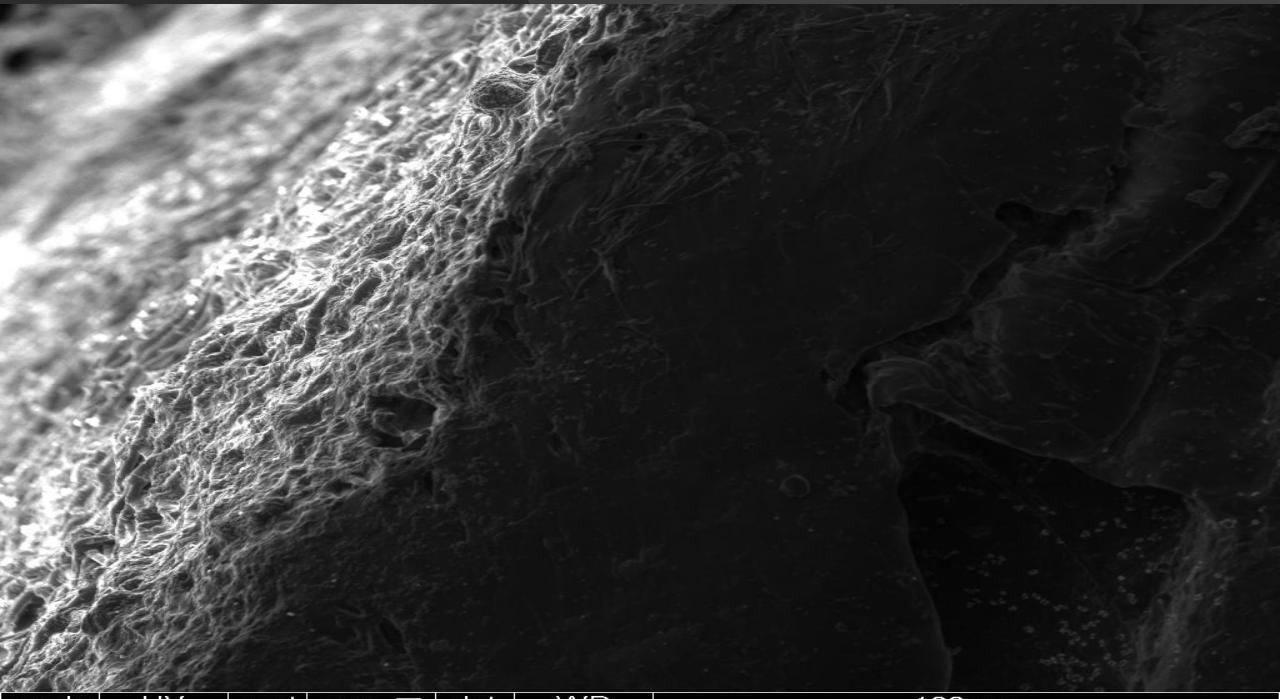


PCL Untreated

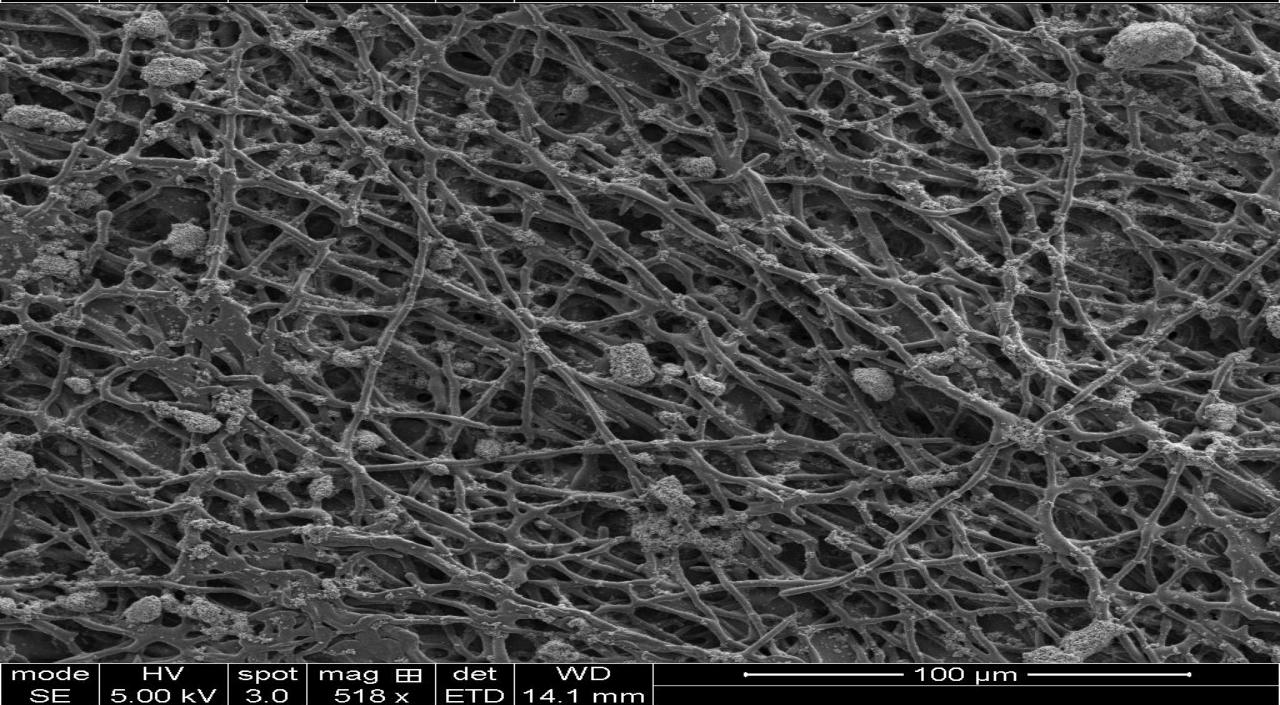




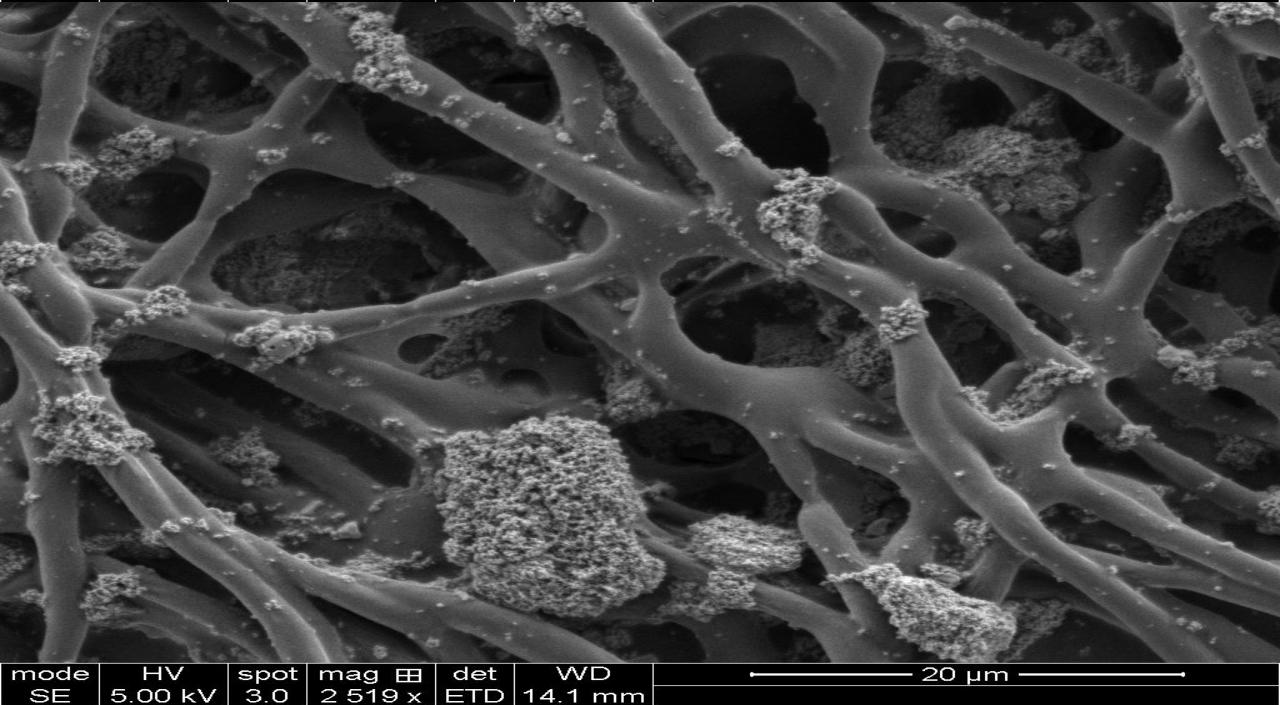
mode SE HV 5.00 kV spot 3.0 mag 65 x det ETD WD 12.0 mm 1 mm



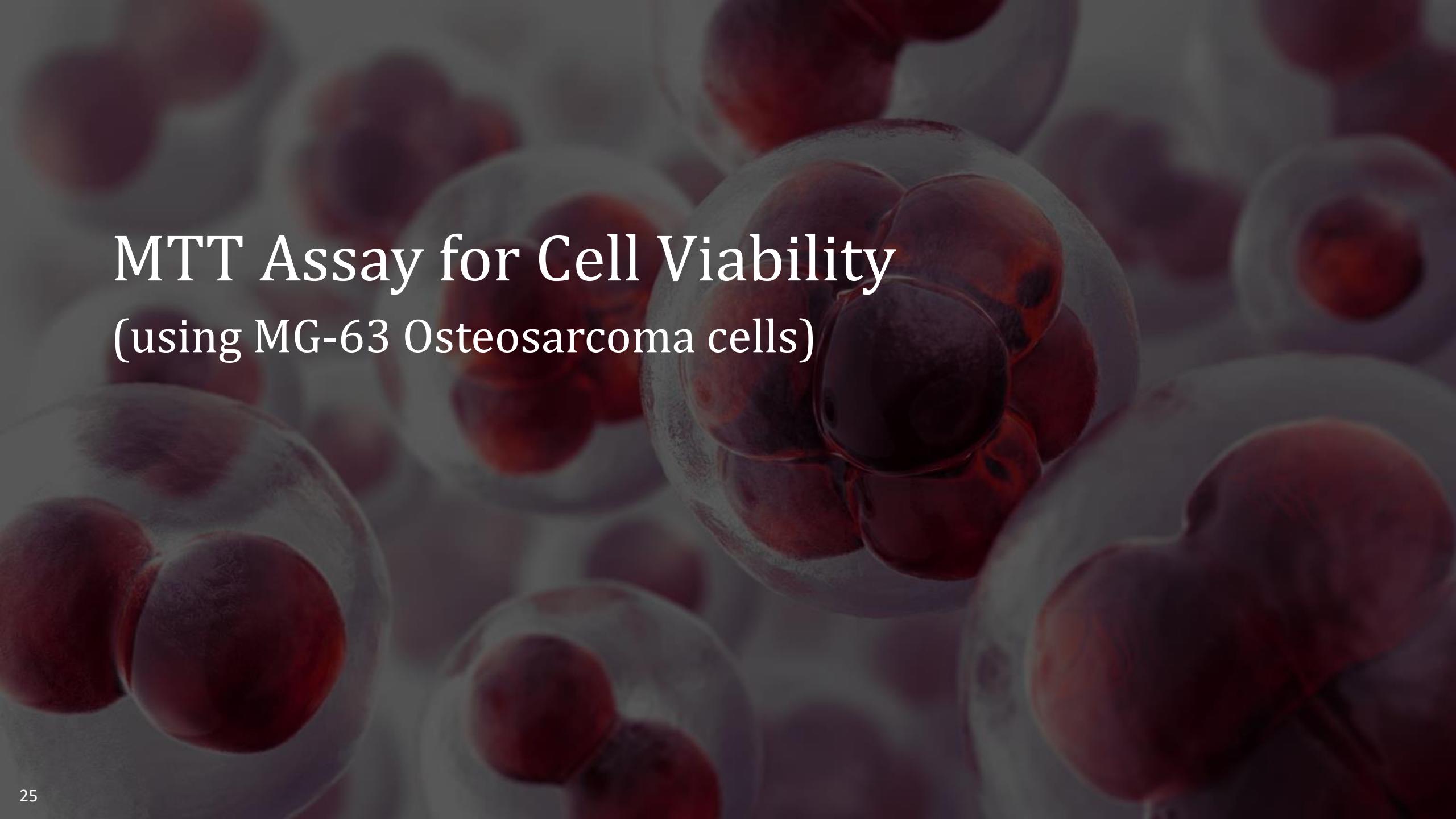
mode SE HV 5.00 kV spot 3.0 mag 679 x det ETD WD 12.2 mm 100 µm



mode SE HV 5.00 kV spot 3.0 mag 518 x det ETD WD 14.1 mm

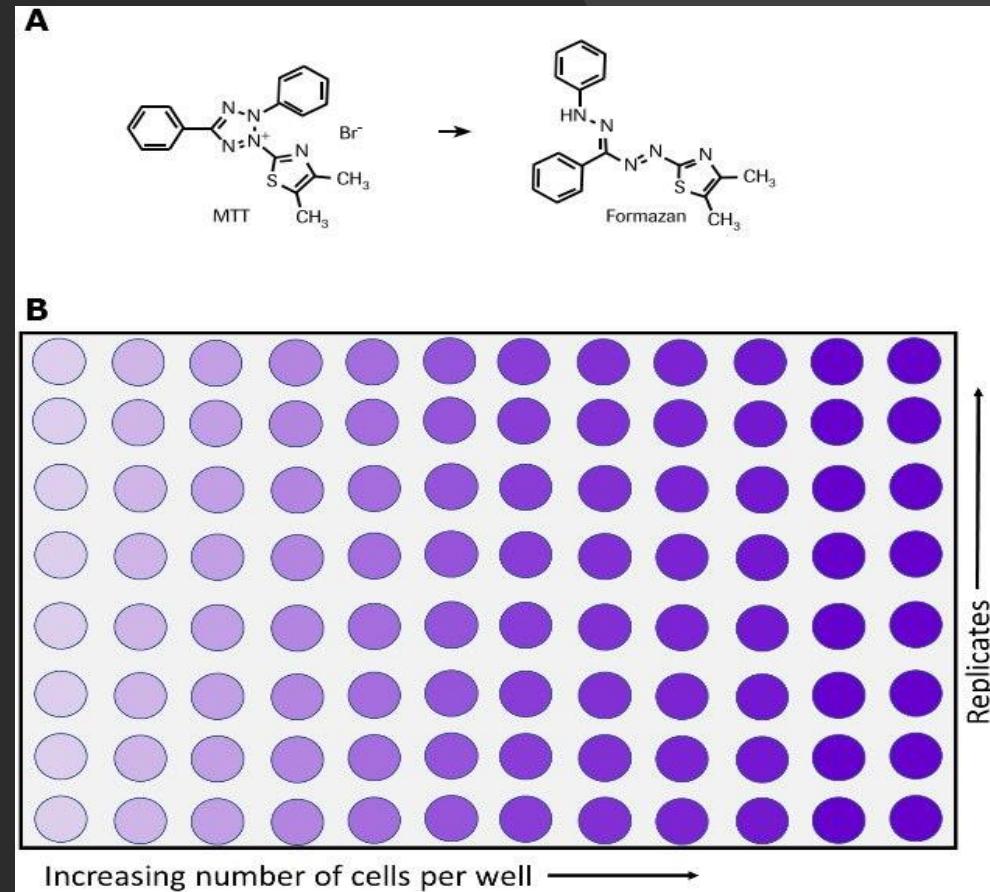
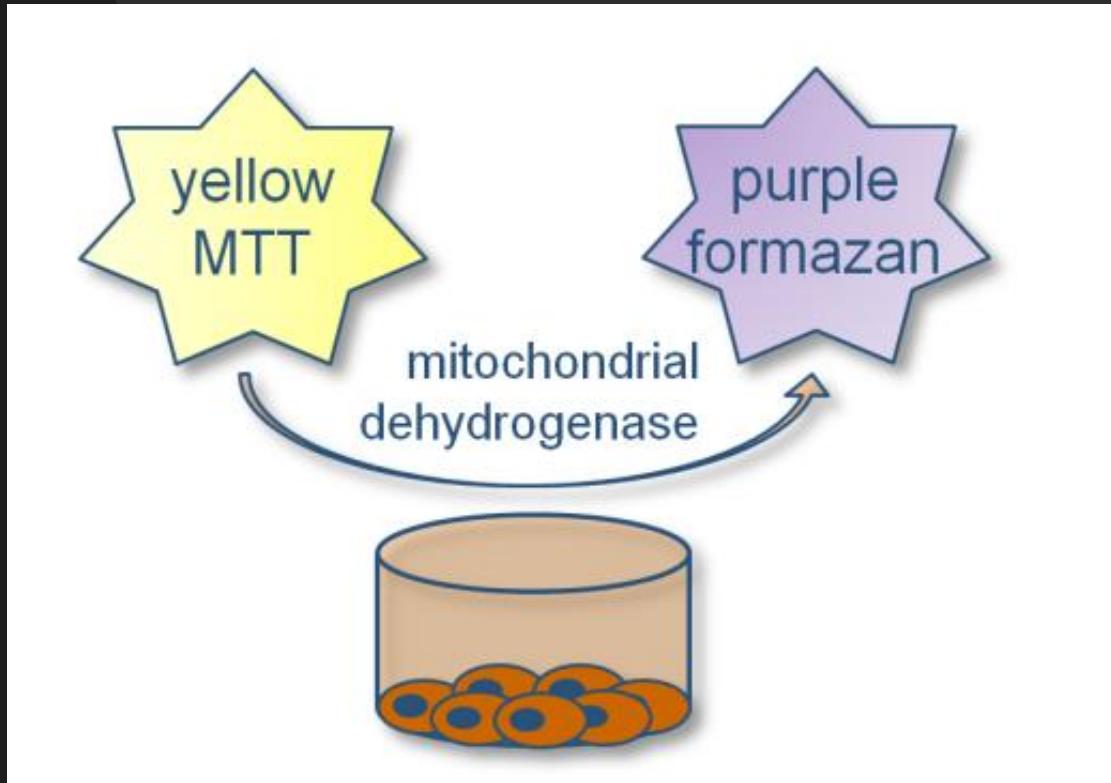


mode SE HV 5.00 kV spot 3.0 mag 2519 x det ETD WD 14.1 mm

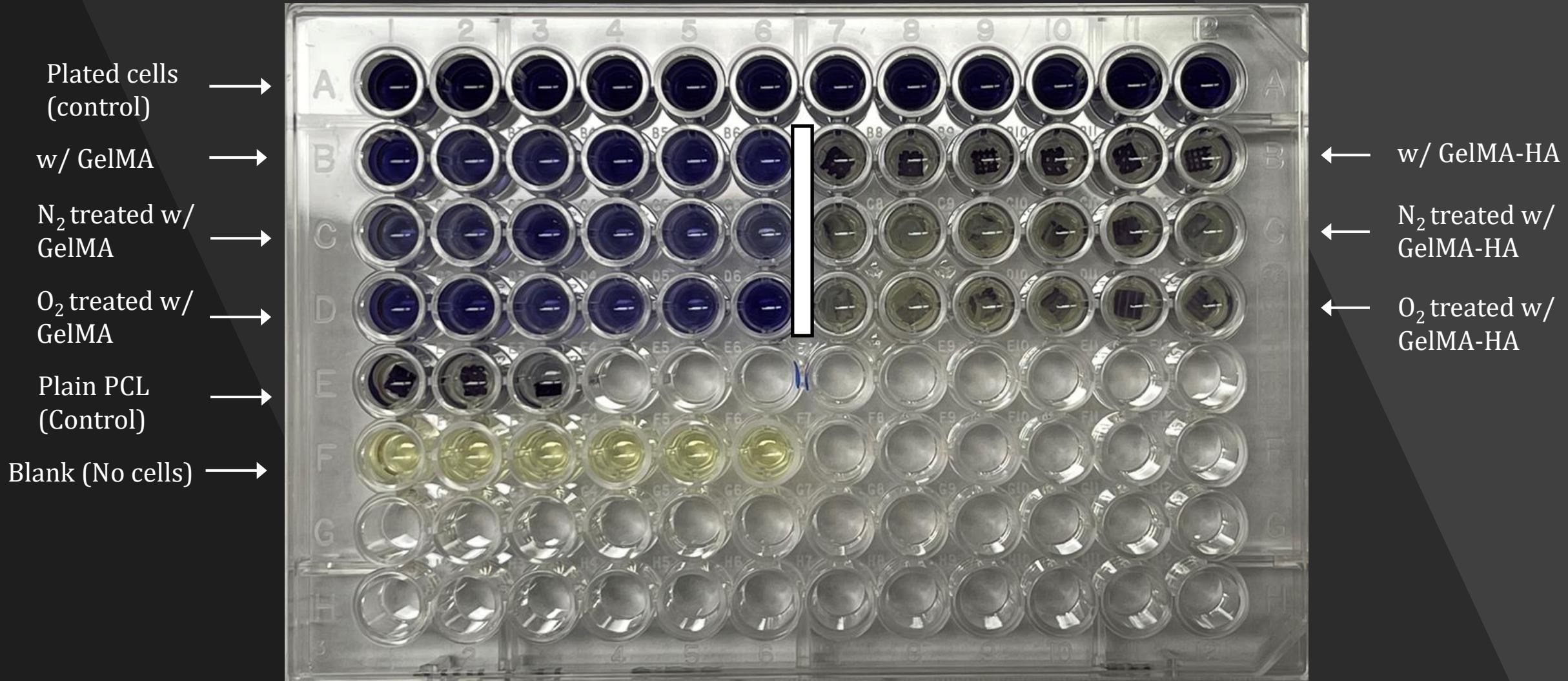


MTT Assay for Cell Viability (using MG-63 Osteosarcoma cells)

- Cell mitochondria convert MTT into formazan crystals, causing a change in color.
- This allows for mitochondrial activity to be directly determined by an absorbance spectrum.

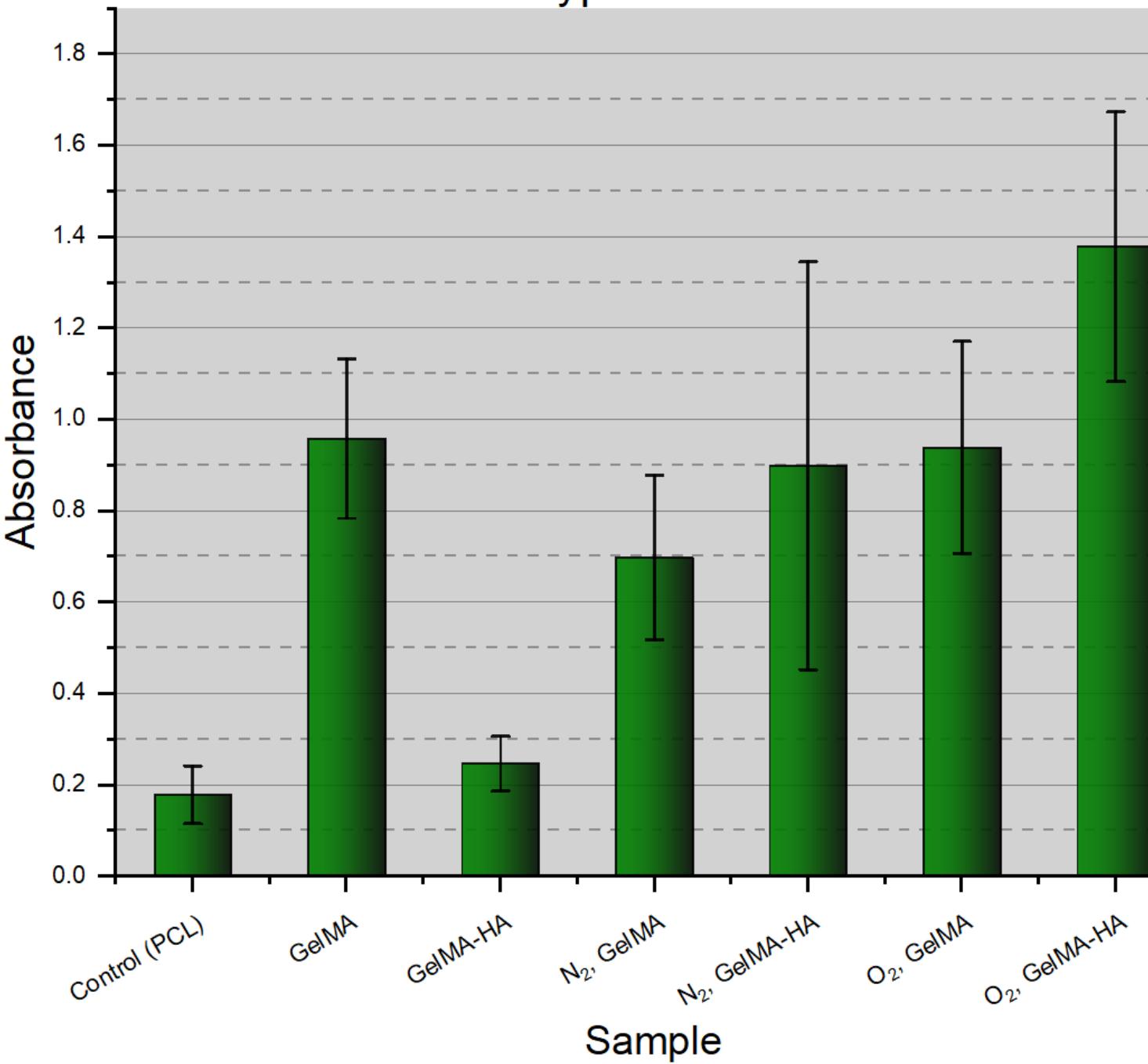


van Meerloo J., Kaspers G.J.L., Cloos J. (2011) Cell Sensitivity Assays: The MTT Assay. In: Cree I. (eds) Cancer Cell Culture. Methods in Molecular Biology (Methods and Protocols), vol 731. Humana Press. https://doi.org/10.1007/978-1-61779-080-5_20
<https://www.sigmaldrich.com/US/en/technical-documents/protocol/cell-culture-and-cell-culture-analysis/cell-counting-and-health-analysis/cell-proliferation-kit-i-mtt>
<https://www.eurofins.de/medizinprodukte-pruefungen/validierte-methoden/mtt-test/>



Higher
absorbance
=
Greater cell
viability

Scaffold Type vs. Absorbance



Summary

- What we did
 - Produced a unique type of scaffold for bone regeneration
 - Successfully integrated hydrogel with scaffold
 - Discovered unforeseen, adverse effects of LTP treatment on mechanical properties
 - Showed an unexpected increase in cell viability for GelMA over GelMA-HA
 - Successful, interesting questions, should be explored further
- What I learned
 - SolidWorks CAD software
 - 3d-printing
 - Analysis techniques
 - X-Ray Photoelectron Spectroscopy (XPS)
 - Water Contact Angle
 - Fourier-Transform Infrared (FTIR) Spectroscopy
 - Rheology
 - Scanning Electron Microscopy (SEM)
 - Hydrogel synthesis
 - Electrospinning
 - OriginLab plotting software

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Gerardo Hernandez-Moreno

Shruti Sanas

Dr. Paul Baker

Dr. Kiran Adhikari

Renjith Rajan

Charita Cadenhead

Mark Case

Amanda Watkins

