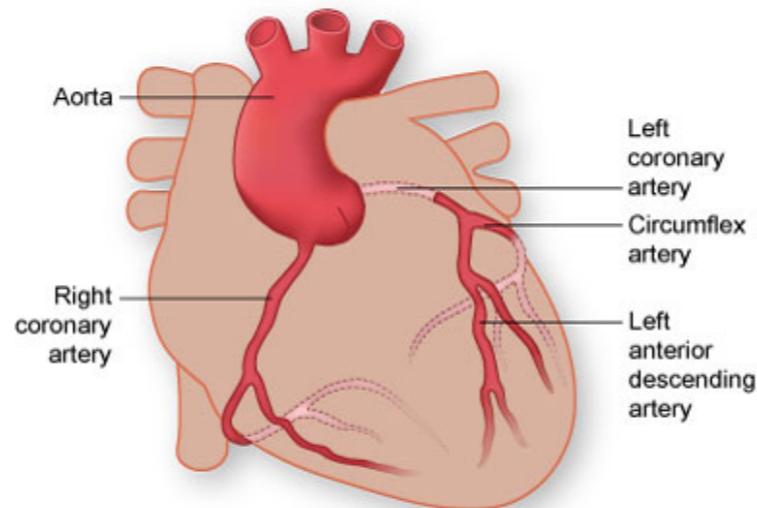


DeepCA:

Deep Learning-based 3D Coronary Artery Tree Reconstruction from Two 2D Non-simultaneous X-ray Angiography Projections



Yiying Wang, Abhirup Banerjee, Robin P. Choudhury, Vicente Grau

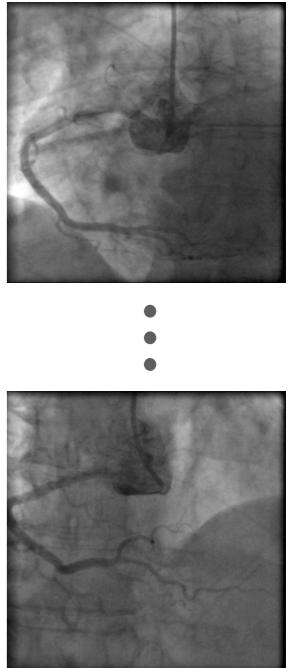
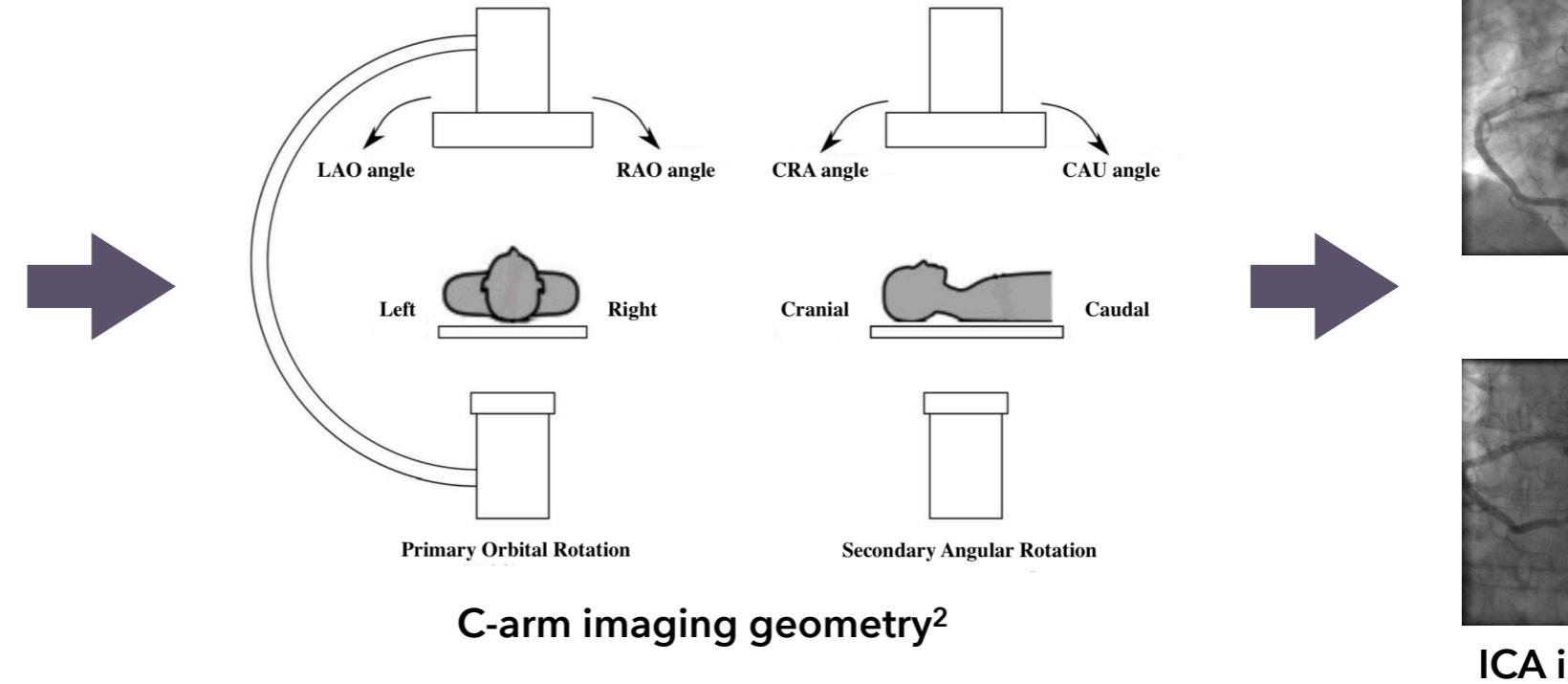
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BACKGROUND

X-RAY INVASIVE CORONARY ANGIOGRAPHY (ICA)



Siemens single-plane C-arm¹



ICA images

- Cardiovascular diseases are the most common cause of death worldwide, representing **32%** of all global death³
- ICA acquires **2D** projections of the coronary artery tree (based on C-arm) and is the gold standard during **cardiac interventions**
- Around **250,000** coronary angiograms are performed across the UK every year⁴

¹ Siemens Healthineers Official Website, Accessed: 22/01/2025

³ World Health Organisation, Accessed: 22/01/2025

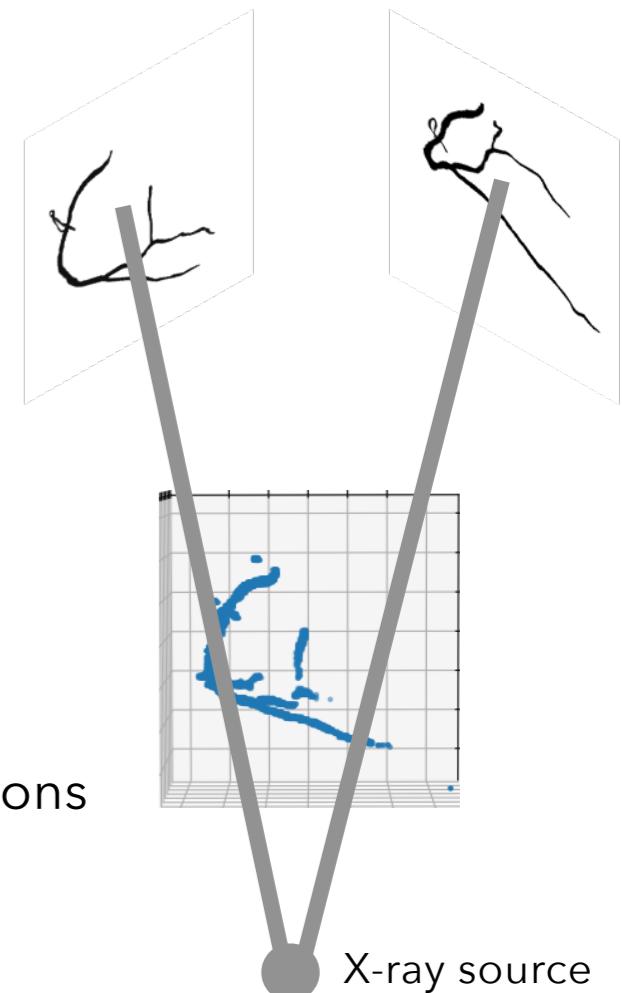
² Kausch et al., 2020

⁴ British Heart Foundation, Accessed: 22/01/2025

MOTIVATION

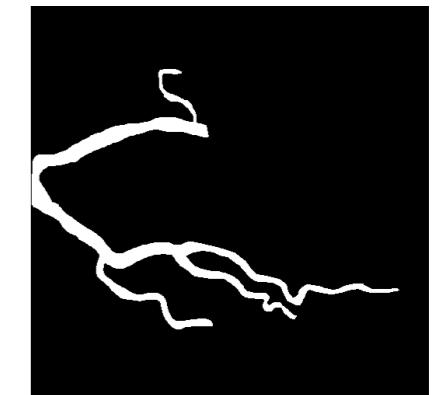
Doing **3D coronary artery tree reconstruction from two ICA images** helps:

- Reduce the likelihood of subjective interpretation of 3D geometry from 2D projections
- Reduce extra contrast injected and extra X-ray radiation dose exposed
- **Deep Learning** helps:
 - 3D reconstruction in real time
 - **Implicitly compensate** for the non-rigid cardiac and respiratory motions



CHALLENGES

- **Non-rigid** cardiac and respiratory motions due to **non-simultaneous image acquisition**, causing vessels to misalign between projections
- Possible patient and device movements between non-simultaneous scans
- Foreshortening, vessel overlap and complex vessel shape
- Only **two** projections acquired and some parts of the vessels in projection images may be incomplete
- Intensity values in projections do not provide additional information due to contrast injected
- **No 3D ground truth** and the number of real clinical 2D ICA data is also **limited**



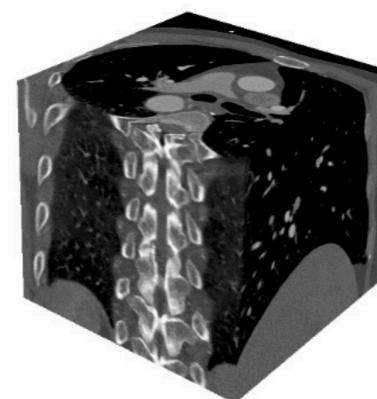
RELATED WORK

- Traditional Methods:
 - Usually require substantial manual annotations
 - Cannot handle non-rigid cardiac motion
- Deep Learning Approaches:
 - Based on synthetic data or Coronary Computed Tomography Angiography (CCTA) data only
 - Use real ICA data from bi-planar scans
 - None of which suffers from **non-rigid motion** between projections

DATA

REAL CCTA DATA

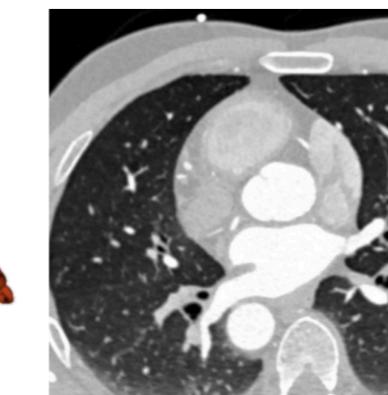
- Issues:
 - No public ICA image datasets with projection geometry information
 - Hard to build the accurate 3D coronary artery tree ground truth even given several real 2D angiograms
- Solution:
 - Public datasets¹ of segmented CCTA data of 1000 patients containing both right coronary artery (**RCA**) and the left anterior descending artery (LAD)



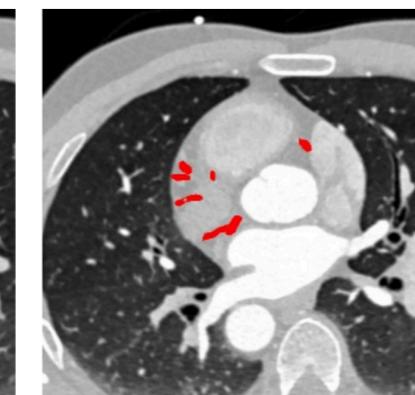
CT



Label



CT slice



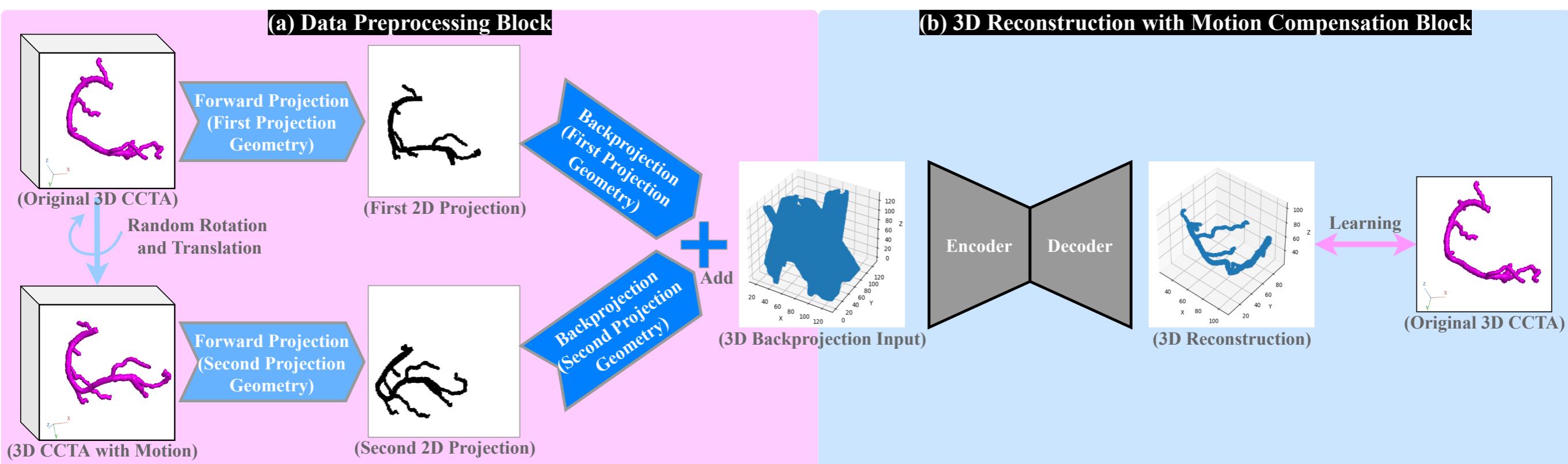
Labels in CT slice

¹ Zeng et al., 2023



METHOD

OUR PROPOSED PIPELINE



(a) Data preprocessing block:

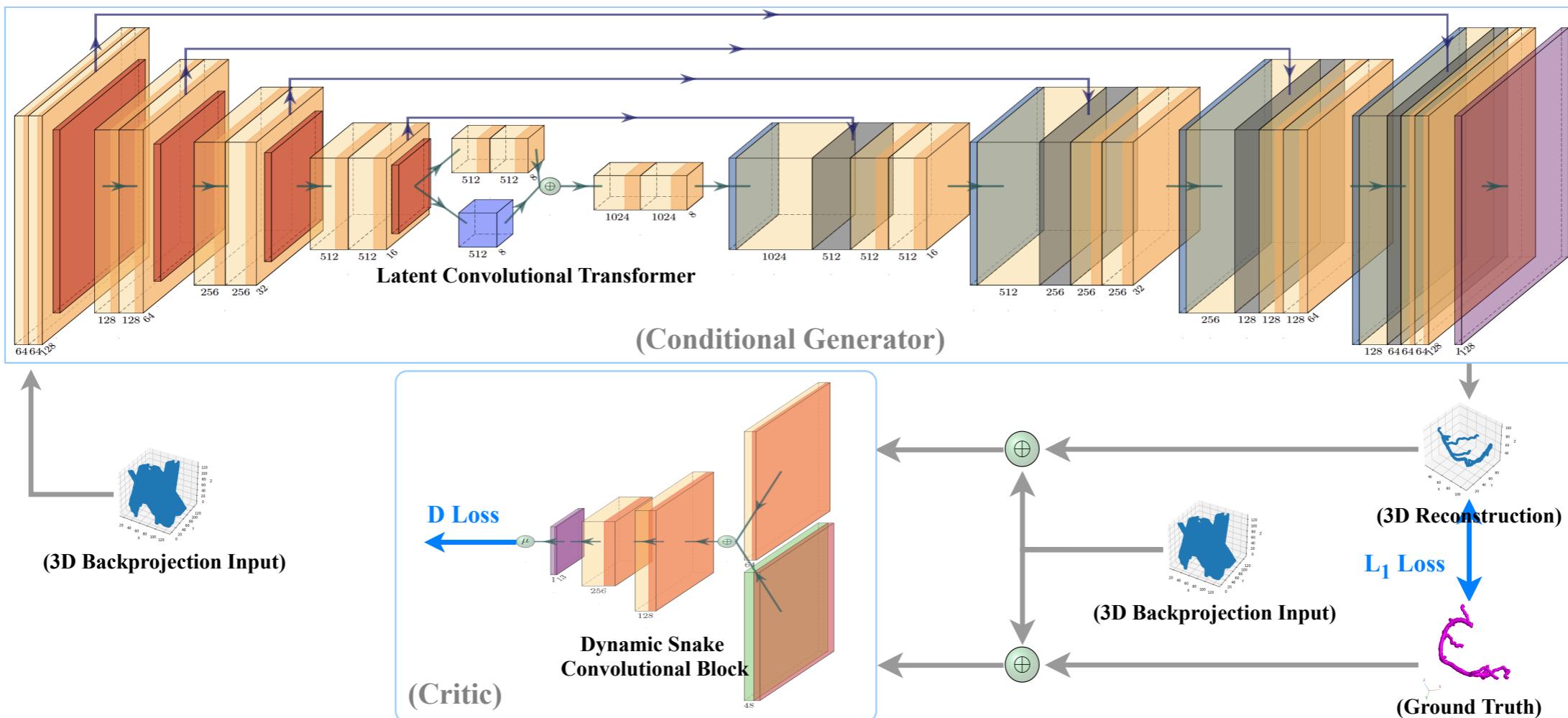
- Two simulated projections from CCTA data, including simulated motion
- Model input via performing backprojection on two simulated projections

(b) 3D reconstruction with motion compensation block:

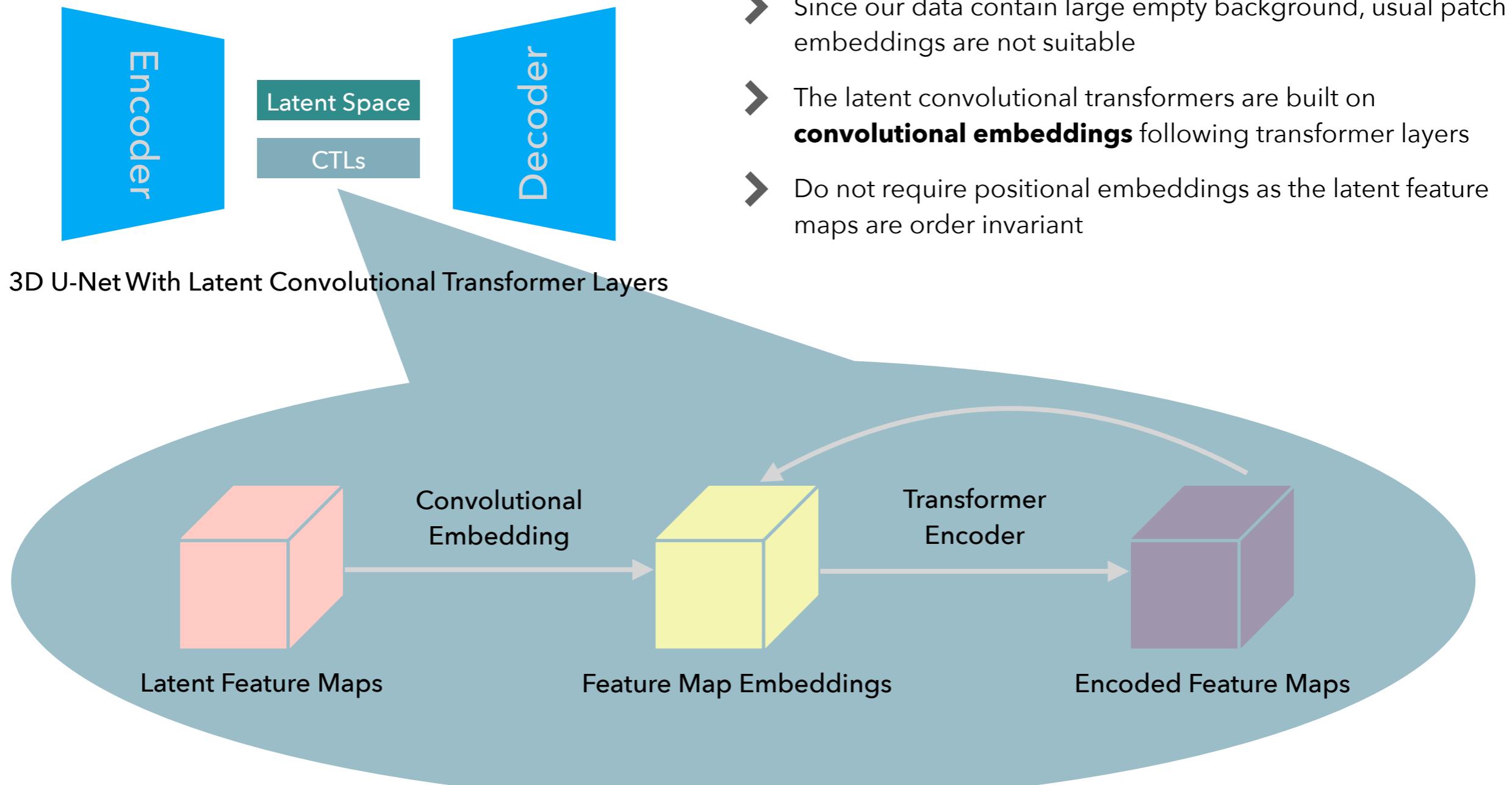
- A deep neural network for 3D coronary artery tree reconstruction

OUR PROPOSED MODEL

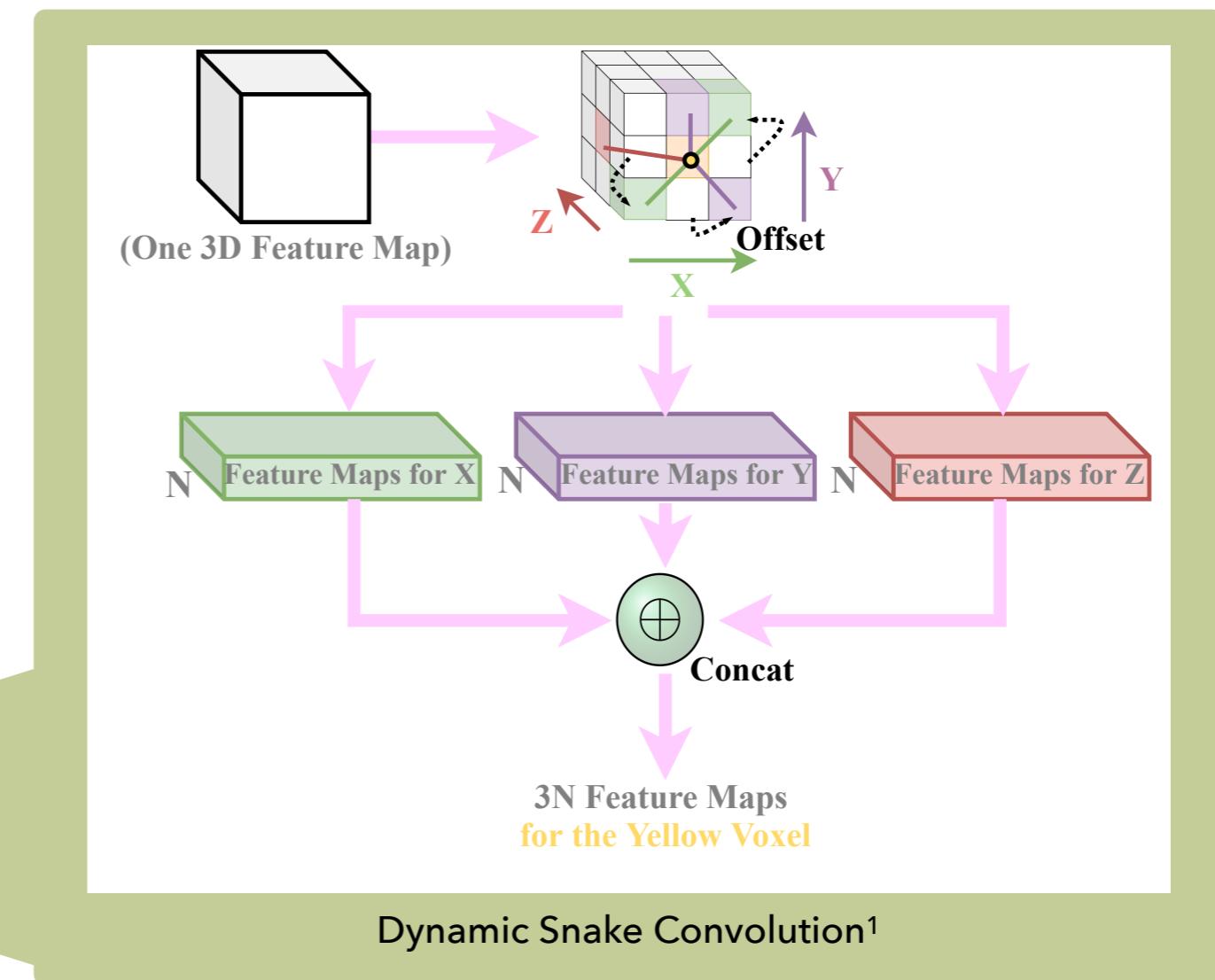
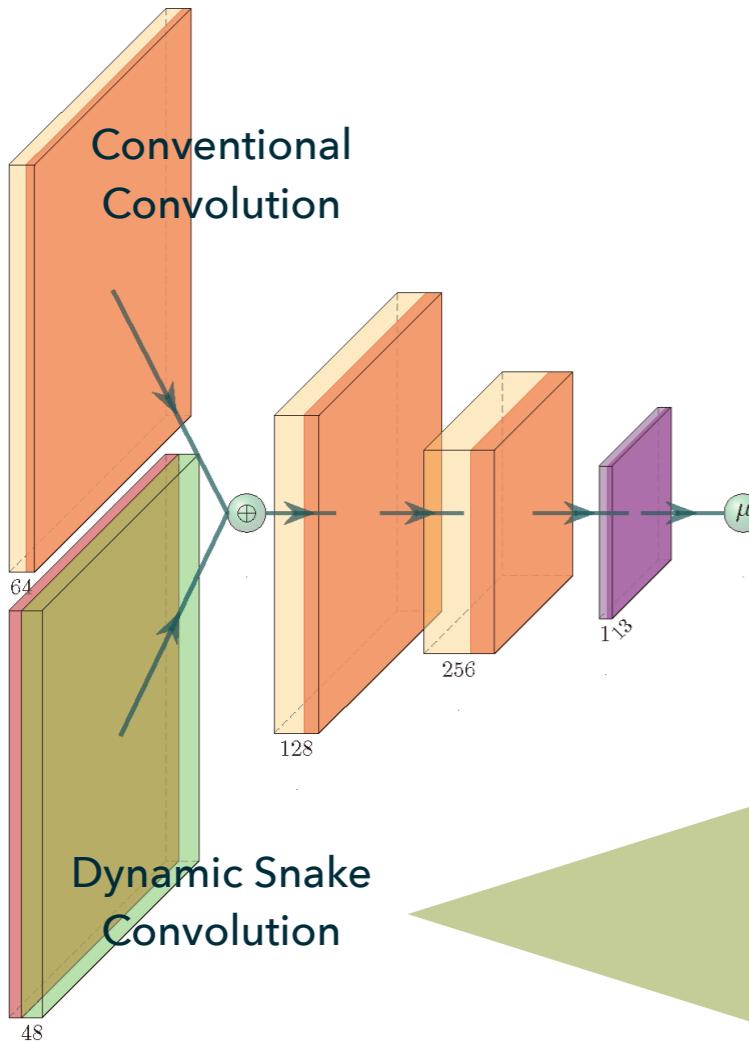
- Based on Wasserstein conditional generative adversarial network with gradient penalty (**WGP**), latent convolutional transformer layers (**CTLs**), and a dynamic snake convolutional critic (**DSCC**).



LATENT CONVOLUTIONAL TRANSFORMERS



DYNAMIC SNAKE CONVOLUTIONAL CRITIC



➤ The proposed critic can effectively **distinguish vessel tubular structures**:

- **Dynamic snake convolution** to extract global **tubular** features
- Traditional convolution to extract essential local features



EVALUATION

DATASETS

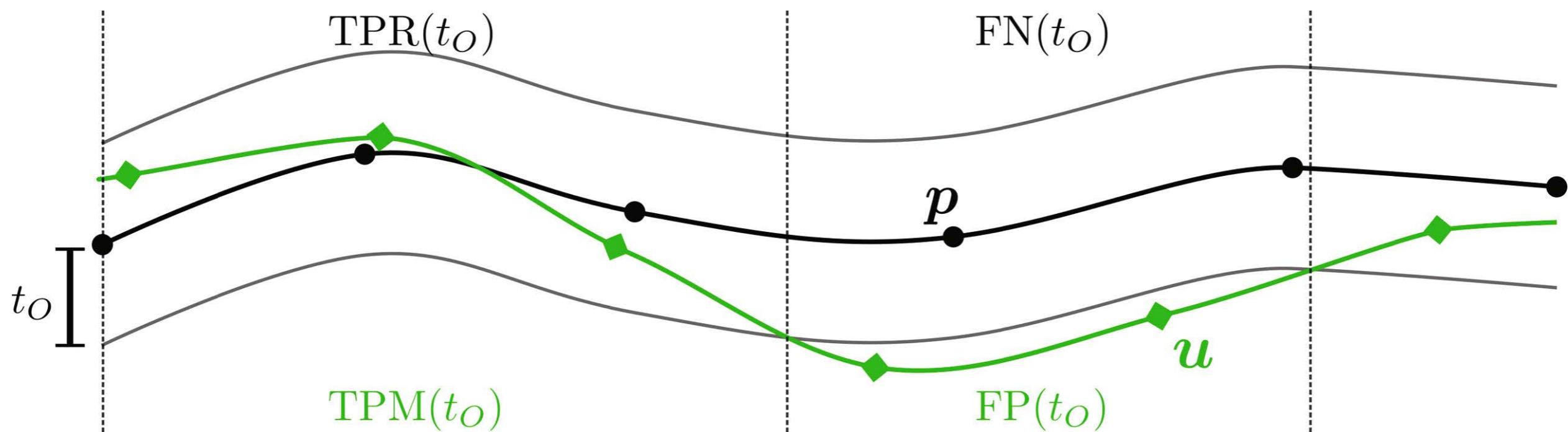
- We use **a public CCTA dataset**, ImageCAS¹, containing 3D binary segmented coronary artery trees for training in our study.
- We also collect **a clinical ICA dataset** of 8 patients for evaluation, who were admitted at the Oxford John Radcliffe Hospital and provided informed consent.

¹ Zeng et al., 2023

METRICS

- **Overlap using a sweeping distance threshold $Ot(t_0)$** ¹, where points of the prediction (**green**) and ground truth (**black**) vessels are labeled as true and false positives or negatives depending on the sweeping test distance t_0 (mm)
- **Chamfer ℓ_2 distance ($CD(\ell2)$)** for measuring the corresponding prediction errors (mm)

$$Ot(t_0) = \frac{|TPM(t_0)| + |TPR(t_0)|}{|TPM(t_0)| + |TPR(t_0)| + |FN(t_0)| + |FP(t_0)|}$$



¹ Çimen et al., 2017

EVALUATION PROCESS

- For the CCTA test dataset, validate 3D results directly after **rigidly registering** the ground truth to the predicted reconstruction
- For real clinical ICA data:
 - Measure the **Dice** score (same as $Ot(0)$) between the ICA data and reprojections of our reconstruction on the **first** projection plane
 - For the **second** and any **additional** projection planes, compute $Ot(t_0)$ and $CD(\ell 2)$ between the ICA data and reprojections **after rigid registration**

RESULTS

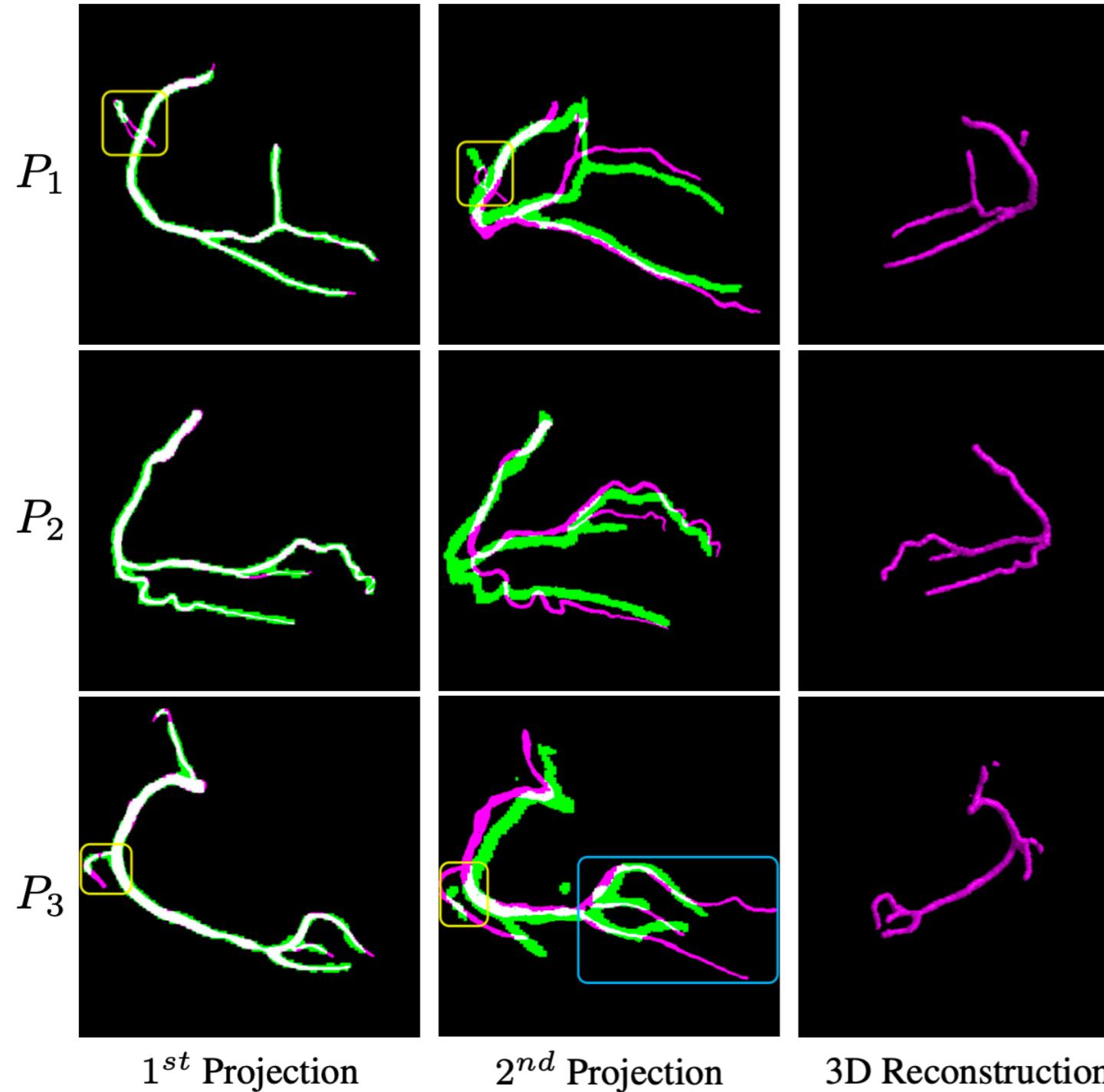
QUANTITATIVE RESULTS

Model	3D CCTA Test Dataset		
	$Ot(1) \uparrow$	$Ot(2) \uparrow$	$CD(\ell_2) \downarrow$
WGP	62.06 ± 10.61	74.38 ± 10.01	3.43 ± 1.29
+CTLs	62.87 ± 11.68	74.39 ± 10.70	3.24 ± 1.23
+DSCC	63.46 ± 10.85	75.14 ± 10.00	3.24 ± 1.23
DeepCA	64.21 ± 10.78	76.25 ± 9.72	3.22 ± 1.20

Quantitative performance in terms of **Ot(t_0)** (%) and **CD(ℓ_2)** (mm) for 3 ablation models (**left**) and 4 baseline models (**bottom**)

Model	3D CCTA Test Dataset			2D Real Clinical ICA Dataset (Unseen Domain)						
	$Ot(1) \uparrow$	$Ot(2) \uparrow$	$CD(\ell_2) \downarrow$	Dice \uparrow	$Ot(1) \uparrow$	$Ot(2) \uparrow$	$CD(\ell_2) \downarrow$	$Ot(1) \uparrow$	$Ot(2) \uparrow$	$CD(\ell_2) \downarrow$
U-Net++	51.99 (± 12.17)	64.75 (± 13.28)	4.64 (± 2.01)	65.42 (± 6.68)	22.97 (± 10.82)	31.05 (± 12.76)	12.79 (± 4.61)	25.25 (± 18.40)	39.37 (± 20.75)	8.49 (± 3.26)
U-Net+++	55.10 (± 10.72)	68.69 (± 10.96)	4.49 (± 1.67)	62.23 (± 9.49)	22.27 (± 8.30)	30.19 (± 10.51)	12.20 (± 3.77)	32.92 (± 23.99)	42.37 (± 26.30)	7.70 (± 1.59)
Dynamic Snake Convolution Net	61.74 (± 14.28)	72.21 (± 13.31)	3.49 (± 1.68)	83.59 (± 4.01)	30.66 (± 11.30)	42.74 (± 11.68)	7.81 (± 2.19)	53.26 (± 6.74)	67.90 (± 4.77)	3.92 (± 0.48)
Convolutional Vision Transformer GAN	61.53 (± 11.49)	73.71 (± 10.75)	3.51 (± 1.36)	76.84 (± 5.73)	32.98 (± 12.29)	44.85 (± 15.85)	8.23 (± 3.73)	49.50 (± 0.82)	64.63 (± 3.05)	4.22 (± 0.51)
DeepCA	64.21 (± 10.78)	76.25 (± 9.72)	3.22 (± 1.20)	83.31 (± 4.32)	45.70 (± 6.79)	58.39 (± 8.42)	4.51 (± 1.29)	58.58 (± 4.01)	72.88 (± 0.90)	2.81 (± 0.06)

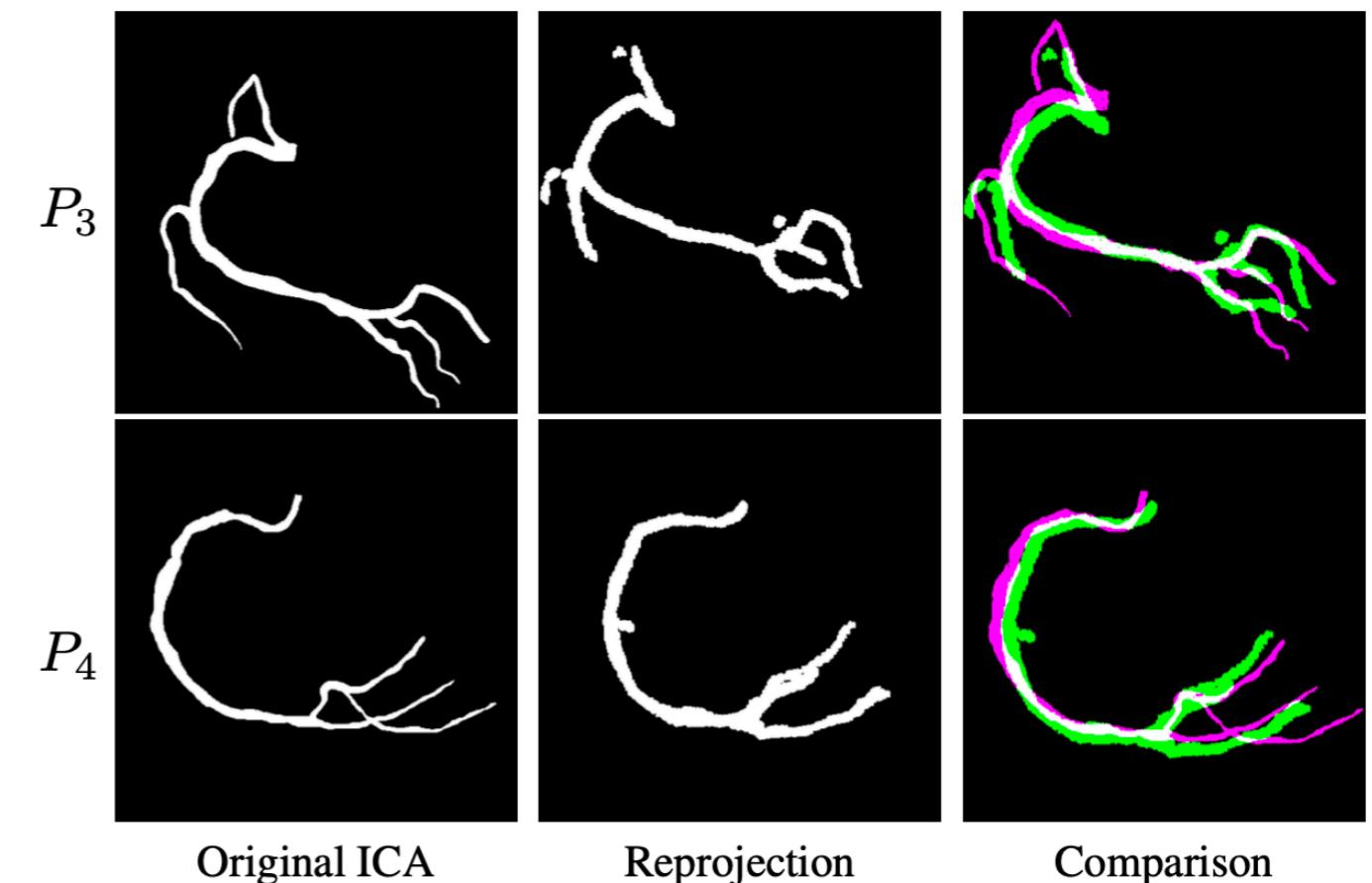
QUALITATIVE RESULTS FOR 1ST & 2ND PROJECTIONS



- From left to right: comparisons of three patients $P_{1,2,3}$ between the real ICA data and our reprojections on the **first** and **second** planes **after rigid registration**, and our DeepCA model's **3D reconstruction**
- Colour **purple** represents ICA data, **green** the reprojeciton, and **white** the overlap

2D EXTRA PROJECTION EVALUATION

- From left to right: original ICA data, reprojections on **the additional projection plane**, and comparisons between them **after rigid registration** of two patients $P_{3,4}$
- Colour **purple** represents ICA data, **green** the reprojection, and **white** the overlap



CONCLUSION

CONCLUSION

- Through simulating projections from CCTA data, we achieve generalisation on non-simultaneous ICA data, **implicitly compensating for non-rigid motion**
- Together with automated coronary vessels segmentation, our model can allow end-to-end automated real-time 3D coronary tree reconstruction during cardiac interventions



THANK YOU



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