

Analysis of Local Field Potentials (Part I & II)

WS 2013/14 | Michael Denker – Introduction Computational Neurosci., RWTH Aachen

Outline

Understanding Local Field Potentials

What is Synchronization?

Synchronization between Local Field Potentials

Fourier Analysis

Coherence

Phase Synchronization

Synchronization between Spikes and Local Field Potentials

Spike-Triggered Averaging

Spike-Field Coherence

Phase Analysis

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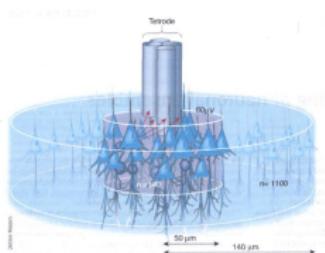
Synchronization between Spikes and Local Field Potentials

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Phase Analysis

Focus: Local Field Potentials



- LFP is the low-pass filtered electrode signal

Buzsaki et al, 2004

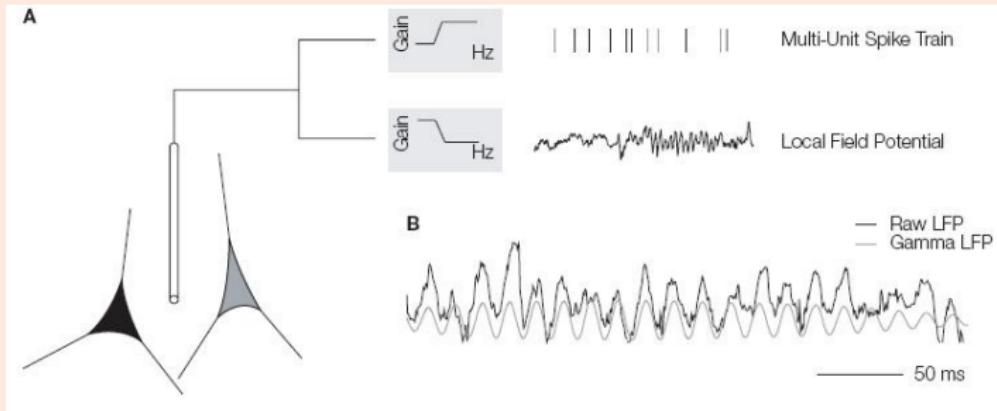
Logothetis and Wandell, 2004

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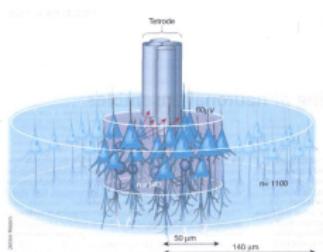
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Obtaining the LFP



Berens et al, 2008

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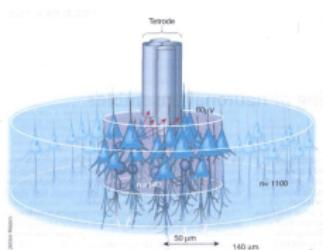


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- **Observed:** Oscillatory structure with dominant frequencies $\lesssim 100 - 300$ Hz

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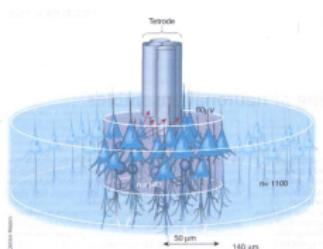
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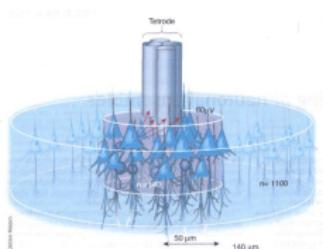
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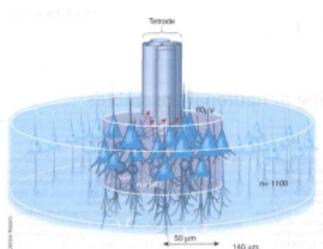
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- ...**but** interpretation of compound LFP is difficult
- Suggested spatial-temporal relationship between LFPs and spikes

Logothetis and Wandell, 2004

Biophysical Origin of LFP

- Under the assumptions of...
 - Quasi-static (< 1 kHz) electric field
(capacitive and inductive effects are negligible)
 - Isotropic extracellular medium
(conductance is a constant scalar, instead of a tensor)

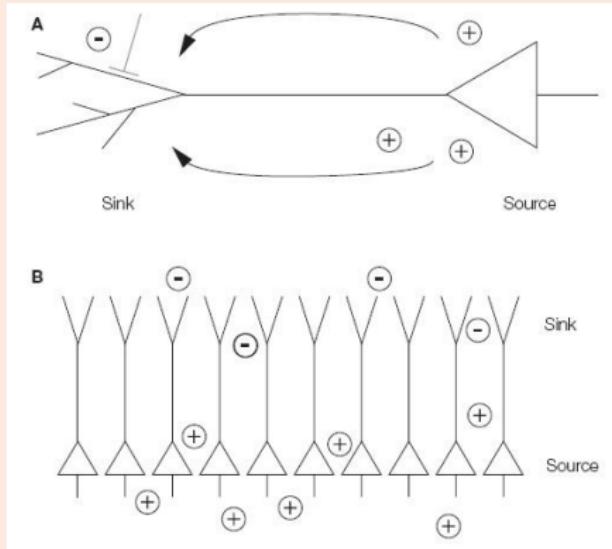
$$\phi(\mathbf{r}) = \sum_i \frac{I_i}{4\pi\sigma|\mathbf{r} - \mathbf{r}_i|}$$

ϕ : field potential I_i : current source at \mathbf{r}_i
 (σ : conductance of extracellular medium)

- Field potential is only dependent on the strength and the position of current sources.
- Current source/sink in extracellular space
 → transmembrane current of neurons

Biophysical Origin of LFP

Biophysical origin of LFP



Johnston and Wu, 1995

Membrane Currents Caused by Neuronal Activities

$$I_m = \frac{V_m}{r_m} + c_m \frac{\partial V_m}{\partial t}$$

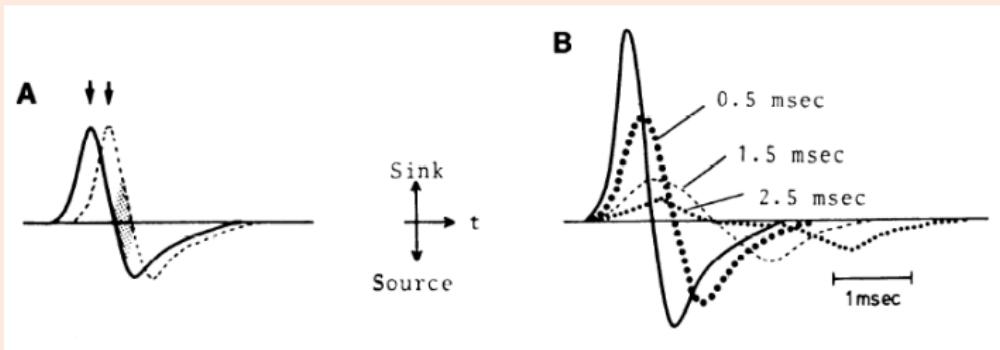
I_m : membrane current V_m : membrane potential

r_m : membrane resistance c_m : membrane capacitance

- Action potentials (somatic, axonal, dendritic)
 - Biphasic in time
 - Easily cancelled out by temporal jitter of multiple APs
- Synaptic potentials (EPSP, IPSP)
 - IPSP is much slower than EPSP
 - Ratio of EPSP- vs. IPSP-related current components = 5:1 (Mitzdorf, 1985)
- EPSPs are essentially the dominant causes of the macroscopic transmembrane current in the brain.

Membrane Currents Caused by Neuronal Activities

Cancellation of currents



Mitzdorf, 1985

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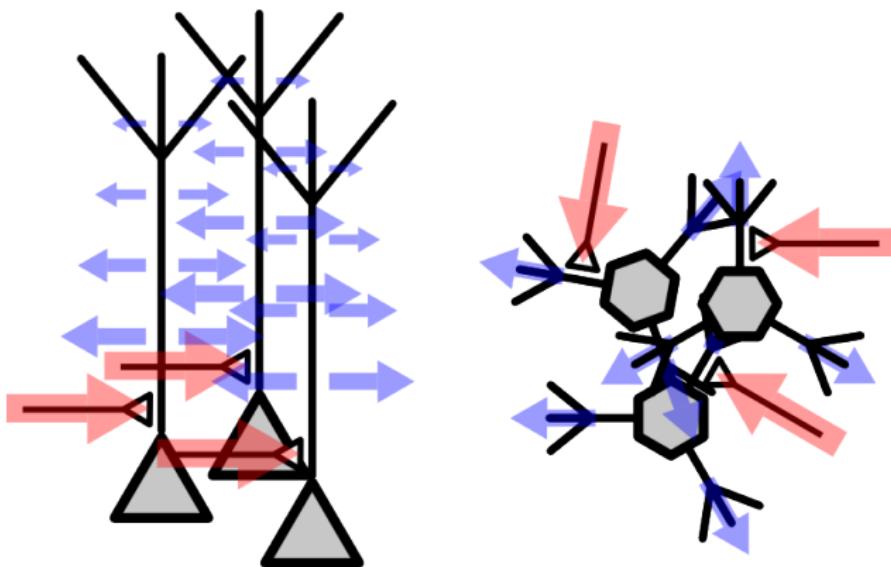
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Effect of Cell Morphology

- Excitatory inputs to pyramidal neurons contribute most to the cortical LFP.



Further Contributions of and by LFPs

Further currents that may contribute to LFP:

- Dendritic calcium spikes
- Resonant properties of the cell, self-sustained oscillations of the membrane potential
- UP/DOWN states during anesthesia or non-REM sleep

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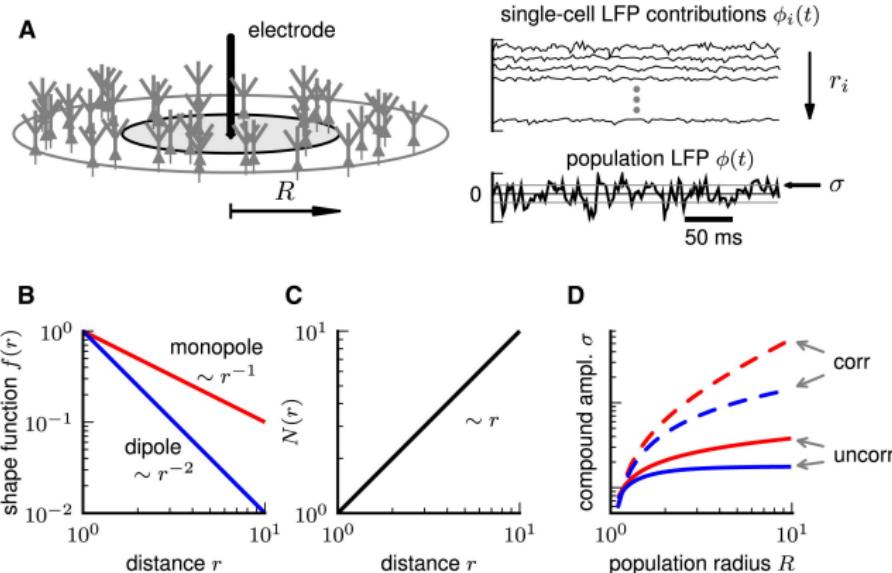
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Ephaptic effects of the local field:

- In how far can the field potential influence the membrane potential of neurons?
- Evidence that constant potentials of realistic magnitude may influence spike timing e.g., Radman et al, 2007; Anastassiou et al, 2011
- Is the LFP an observable of brain dynamics or part of a feedback cycle?

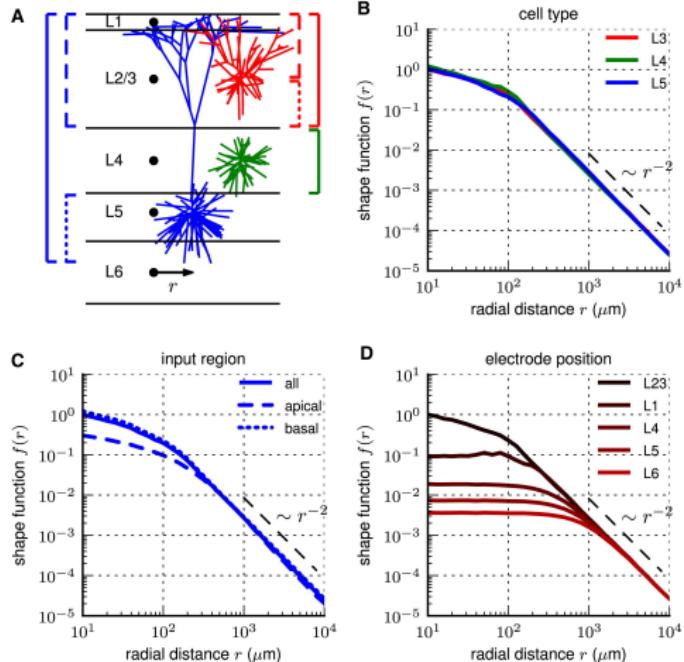
Reach of the LFP



Lindén et al, 2011

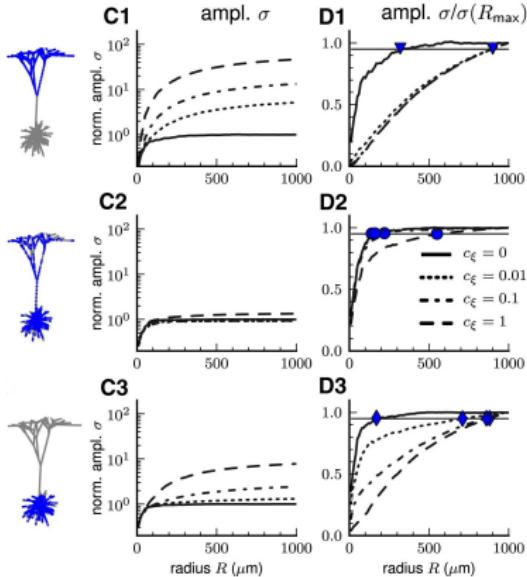
Dependence of LFP reach on cell morphology, synaptic-input distribution, and input correlations

Dependencies of the Reach



Lindén et al, 2011

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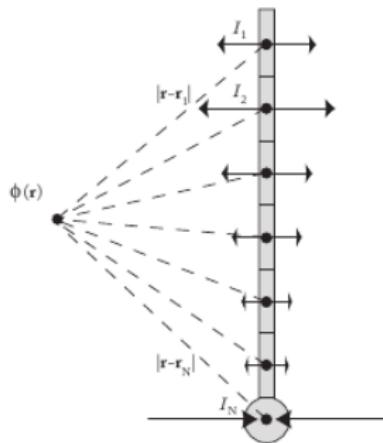


Lindén et al, 2011

Dependencies of the Reach

- Uncorrelated activity OR symmetric cell morphology OR symmetric input distribution:
 $\text{reach} \approx 100, \dots, 300 \mu\text{m}$ (soma layer)
- Correlated activity AND asymmetric cell morphologies (pyramidal cells) AND asymmetric distribution of synaptic inputs (e.g. apical input):
 $\text{reach} \approx \text{spatial extent of correlated activity}$
- **Small correlations** (e.g. shared-input correlations) sufficient to boost LFP reach ($\approx 1 \text{ mm}$)

Current Source Densities

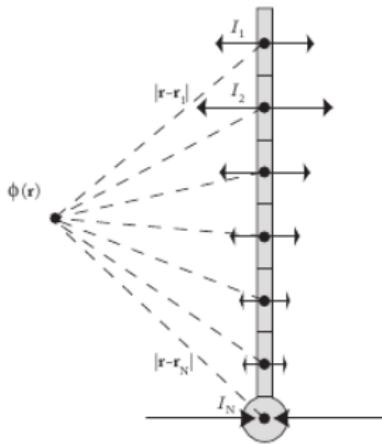


- Forward problem
straight-forward (linear sup.):

$$\phi(\mathbf{r}) = \frac{1}{4\pi\sigma} \iiint_V \frac{C(\mathbf{r}', t)}{|\mathbf{r} - \mathbf{r}'|} d^3 r'$$

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- $C(\mathbf{r}', \mathbf{t}) = \sum_i I_i \delta^3(\mathbf{r} - \mathbf{r}_i)$ is the current source density [A/m^3]

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- Simple CSD estimation formula for electrodes spaced at distance h :

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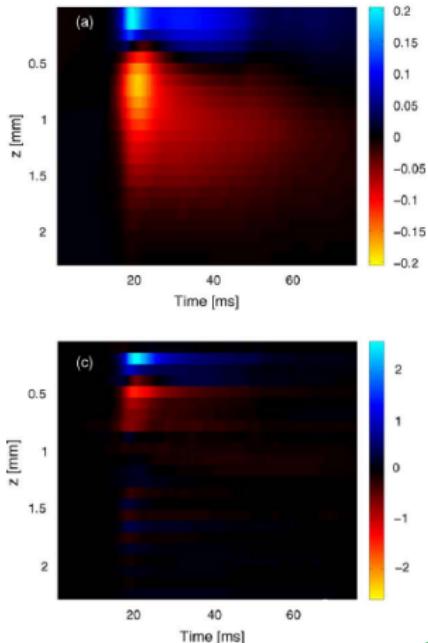
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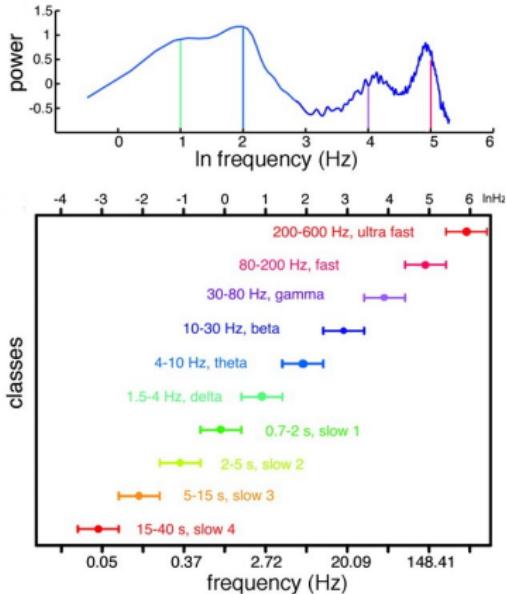
- Problem: Only prediction at $N - 2$ contacts, strong assumptions
- More advanced methods available (e.g., iCSD using a direct inversion of the forward problem (Pettersen et al., 2006)).

Example: Current Source Density in Response to Whisker Deflection in Rat Barrel Cortex



Pettersen et al, 2006

LFP Features: Oscillations



Buzsaki et al, 2004

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- How are such measures related to the system and/or its coupling?

A well-known example: The Millenium Bridge

[Start Millenium Bridge Movie](#)

adapted from: Pikovsky, Rosenblum, Kurths

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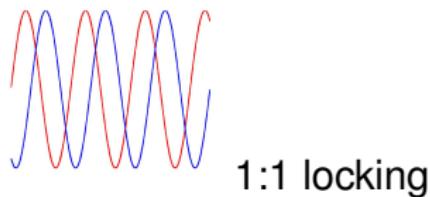
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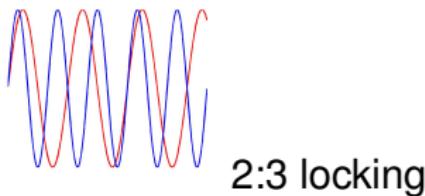
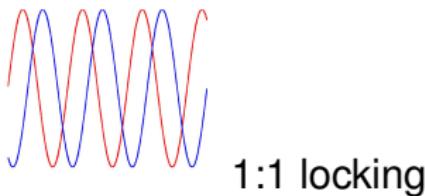
- Critical number of people on the bridge leads to strong vibrations.
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- Instead: **Coupling** between walking pedestrians mediated by bridge leads to **synchronization**

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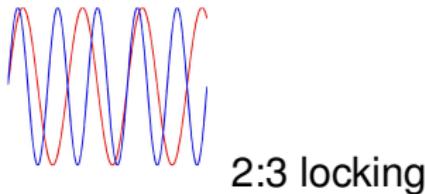
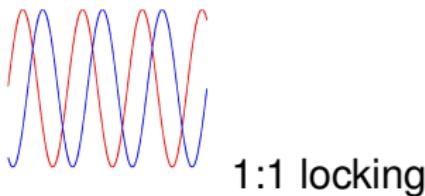
Simplest System: Two Harmonic Waves



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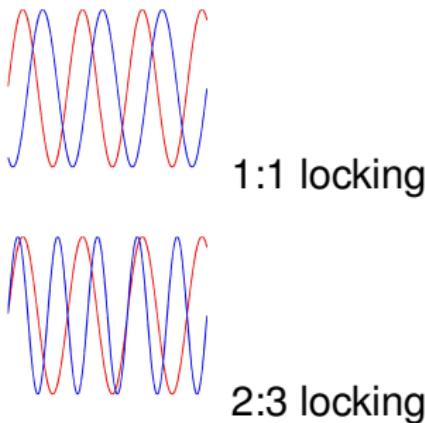


Simplest System: Two Harmonic Waves



Harmonic waves $\sin(\omega_1 t)$ and $\sin(\omega_2 t)$ have $N : M$ -locked frequencies ω

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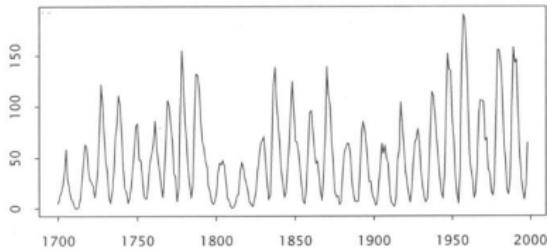
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Harmonic waves $\sin(\phi_1(t))$ and $\sin(\phi_2(t))$ are $N : M$ -locked for fixed differences of their phase ϕ

$$\Delta\phi = (N\phi_1(t) - M\phi_2(t)) \bmod 2\pi = \text{const}$$

Real Signals Are Not Harmonic

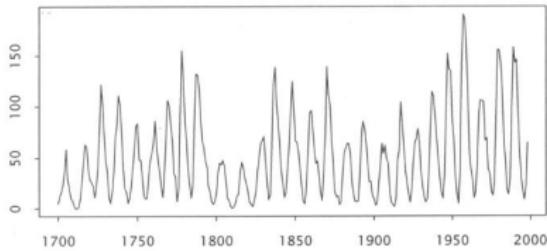
How to determine synchrony for complicated time series?



Rosenblum et al, 1997; Kurths and Pikovski, 2001

Real Signals Are Not Harmonic

How to determine synchrony for complicated time series?



Different **types of synchrony**:

- Complete Synchronization
- Lag Synchronization
- General Synchronization
- Frequency Synchronization
- Phase Synchronization

Rosenblum et al, 1997; Kurths and Pikovski, 2001

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In the following, we will look at two common methods to quantify synchronized time series:

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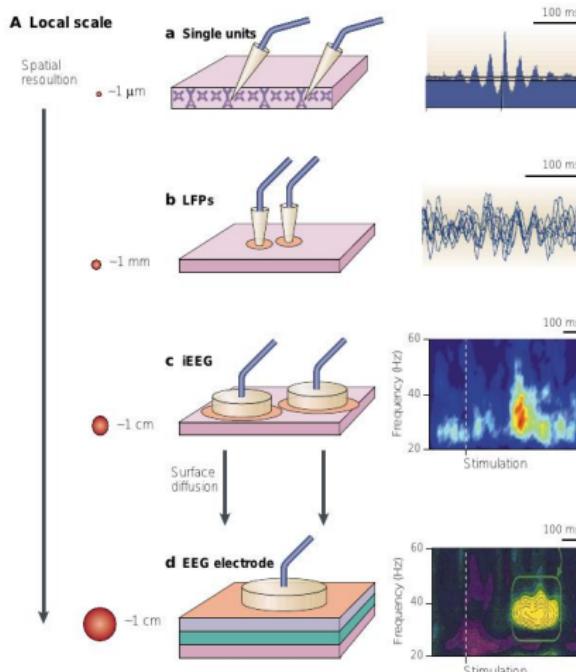
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- ...

Why Study Synchrony in the Brain?



- Measure coorporate activity across brain areas → **functional connectivity**
- Relationship between signals at various mesoscopic and microscopic **scales**
- **Coding** of information in the phase information between signals

Varela et al, 2001

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Decomposing a Signal - Fourier Analysis

- Every (infinite, periodic) signal may be decomposed into an infinite sum of harmonics

$$x(t) = a_0 + \sum_{n=1}^{\infty} (a_n \cos(2\pi f_n t) + b_n \sin(2\pi f_n t))$$

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$$\mathcal{F}(x(t)) = S(f) = |S(f)| \exp(i\theta) = \frac{1}{2\pi} \int x(t) \exp(-2\pi itf) dt$$

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- The magnitude $|S(f)|$ corresponds to the **amplitude** of the harmonic at frequency f , the **phase θ** determines its offset from a cosine

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- The real-valued, squared Fourier spectrum is known as the power spectrum

$$P(f) = S(f)S^*(f) = |S(f)|^2 \exp(i(\phi - \phi)) = |S(f)|^2$$

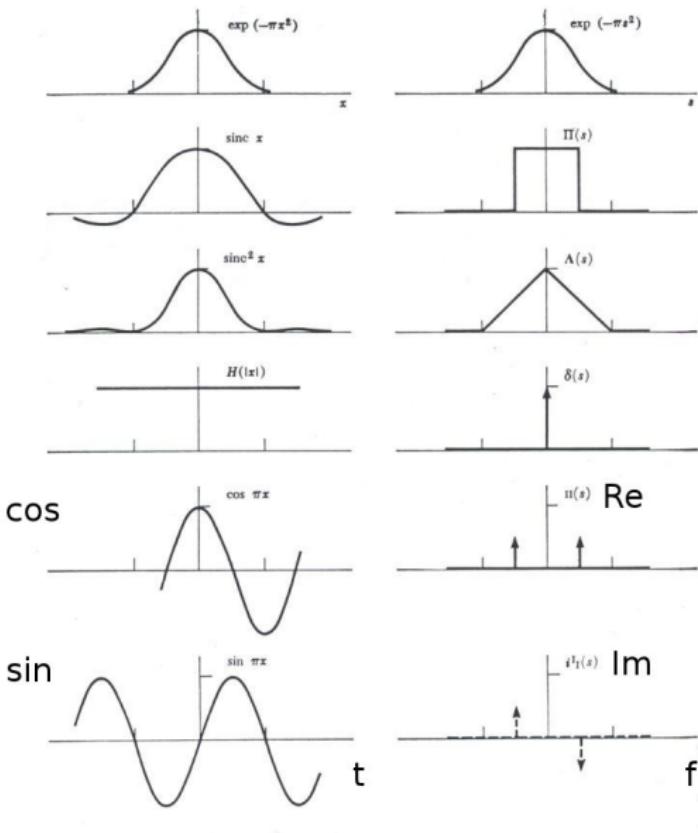
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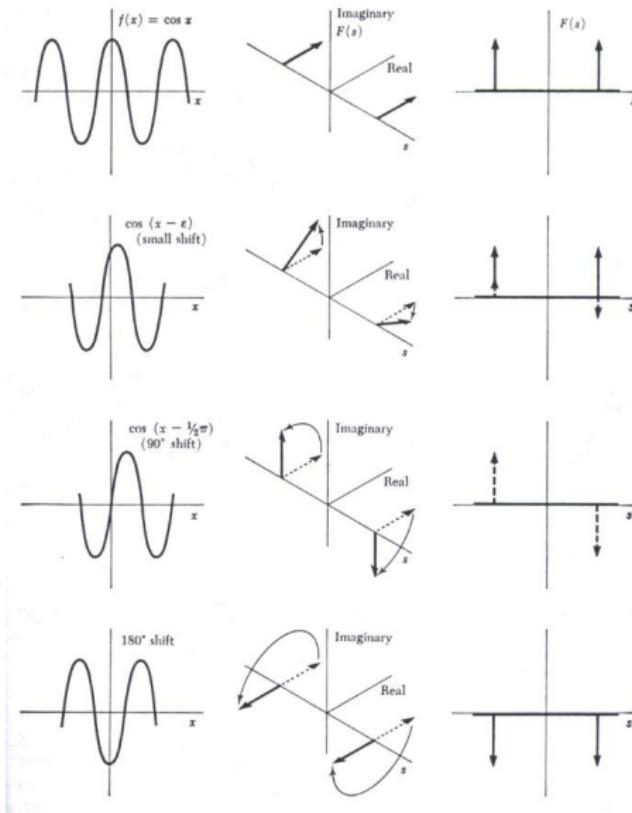
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- In short: Measure of how dominant individual frequencies are present in the signal

Examples of Simple Fourier Transforms



The Phase of the Fourier Transform



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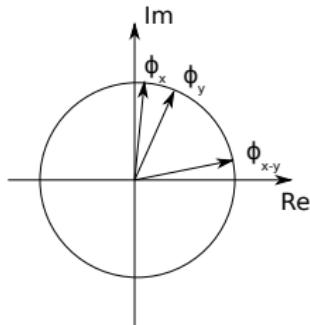
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Cross-spectrum:

$$C_{xy}(f) = S_x(f)S_y^*(f) = |S_x(f)| |S_y(f)| \exp(i(\phi_x - \phi_y))$$



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Cross-coherence:

$$C_{xy}(f) = \langle S_x(f)S_y^*(f) \rangle_{t,n,\Delta f}$$

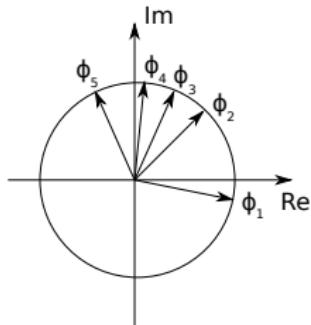
Here, $\langle \cdot \rangle$ denotes an average over time, an average over trials, and/or an average over a small frequency band centered on f

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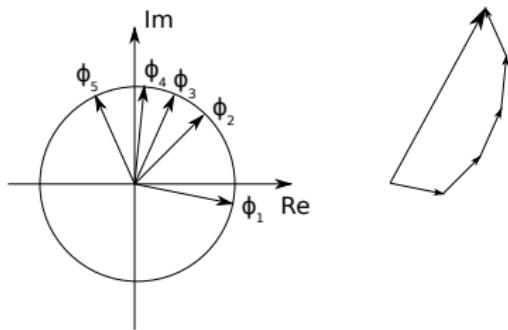


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$$\sigma_{xy}(f) = \left| \frac{C_{xy}(f)}{\sqrt{P_x(f)P_y(f)}} \right|$$

Absolute value of the averaged cross-spectra normalized by the average power content of signals at frequency f

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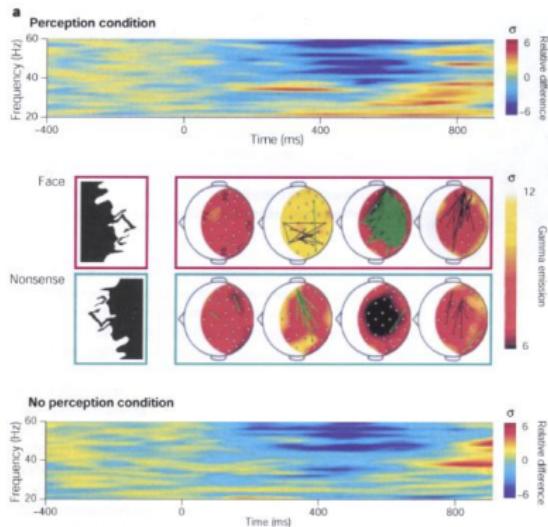
Mean-amplitude normalized coherence index

$\sigma_{xy} = 1 \rightarrow$ Perfect coherence

$\sigma_{xy} \rightarrow 0 \rightarrow$ Incoherent dynamics

Example: Long-distance Synchronization

Face-perception task in macaque EEG recordings results in long-range gamma band synchronization



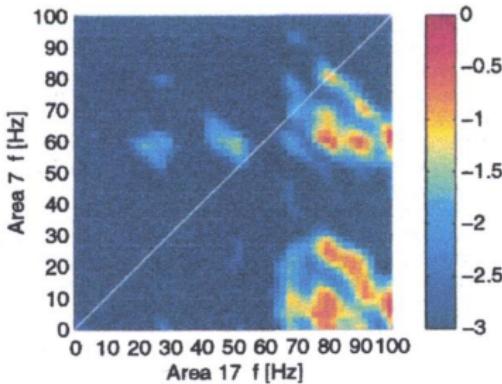
Rodriguez et al, 1999; Varela et al., 2001

Example: Dual Bi-Coherence

Cross-analyze frequencies:

$$C_{xy}(f_1, f_2) = \langle S_x(f_1)S_y(f_2) \rangle_{t,n,\Delta f}$$

$$\sigma_{xy}(f_1, f_2) = \left| \frac{C_{xy}(f_1, f_2)}{\sqrt{P_x(f_1)P_y(f_2)}} \right|$$



v. Stein et al, 2000

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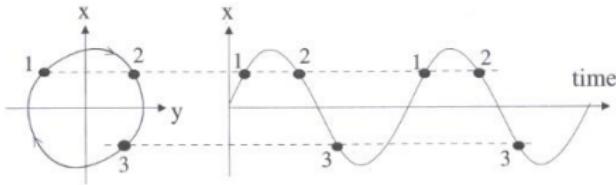
Phase Analysis

Phases in General Oscillating Systems

Consider complicated systems that reflect oscillatory dynamics

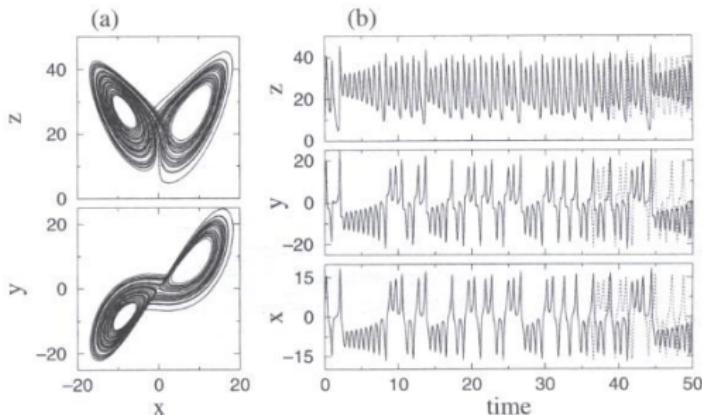
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Phases in General Oscillating Systems

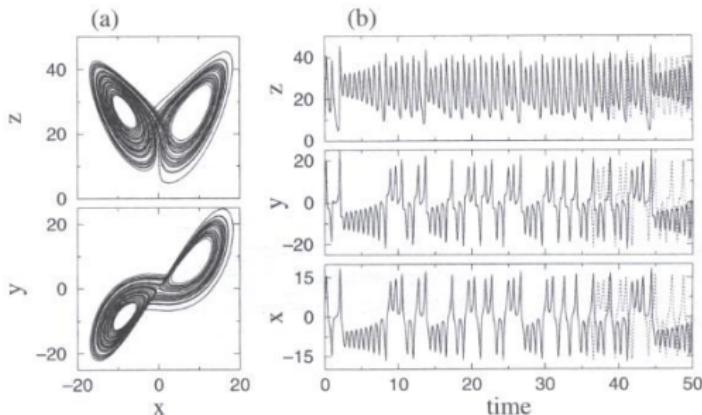
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Kurths, 2001

Phases in General Oscillating Systems

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Kurths, 2001

Task 1: Assign a phase $\phi(t)$ to measured dynamics

Coupling Induces Phase Synchronization

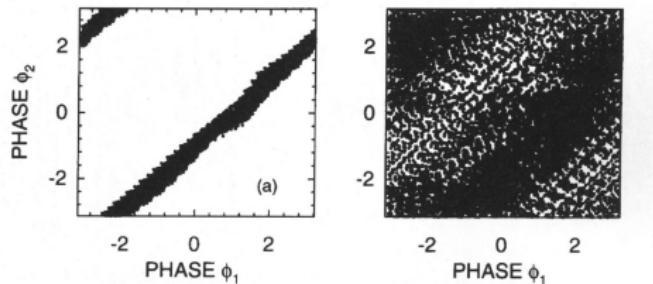
We define $N : M$ phase synchronization between $x_1(t)$ and $x_2(t)$:

$$\Delta\phi = \text{const}_t = (N\phi_1 - M\phi_2) \bmod 2\pi = \text{const.}$$

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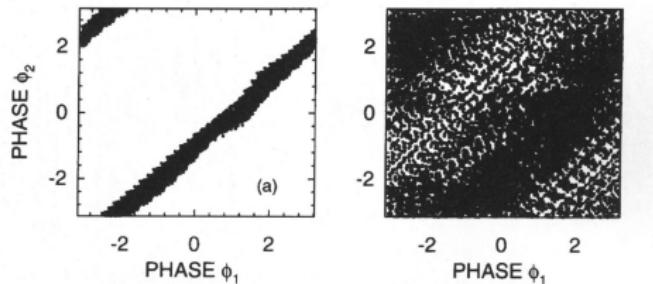


Palus, 1997

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Palus, 1997

Task 1: Assign a phase $\phi(t)$ to measured dynamics

Task 2: Define index to measure **degree of phase synchrony**

Task 1: Obtaining Phase Estimates from Time Series

Method 1: Extract maxima of signal $x(t)$, linear interpolation between maxima from 0 to 2π
→ Simple, but problematic (linearity, maxima detection)

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First exponential localized individual points for phase estimation

Second exponential is a complex rotation that detects instantaneous phase around frequency f

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Method 3: Transform into analytic signal

Task 1: Obtaining Phase Estimates from Time Series

Method 1: Extract maxima of signal $x(t)$, linear interpolation between maxima from 0 to 2π

• Signals but no phase (linearity requires detection)

Which method to use?

Wavelets and Hilbert yield comparable results.

Here: Use analytic signal (Hilbert) approach for simplicity.

Le van Quyen et al, 2001

$$\dots \rightarrow 2\sigma^2 / \dots$$

First exponential localized individual points for phase estimation

Second exponential is a complex rotation that detects instantaneous phase around frequency f

Method 3: Transform into analytic signal

Obtaining Phase Estimates using the Analytic Signal

The Analytic Signal is defined as

$$\tilde{x}(t) = x(t) + i\mathcal{H}[x(t)]$$

via Hilbert Transform

$$\mathcal{H}[x(t)] = \frac{-1}{\pi t} * x(t)$$

Idea: \mathcal{H} yields a signal phase-shifted by $\pi/2$.

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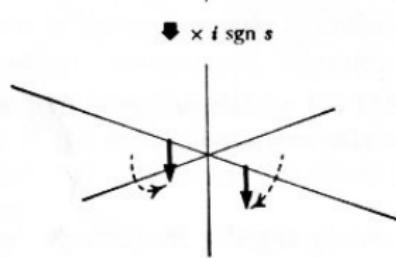
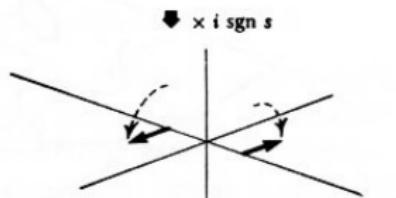
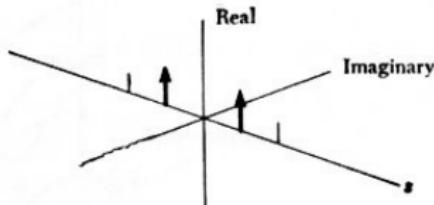
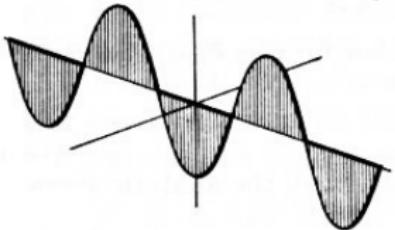
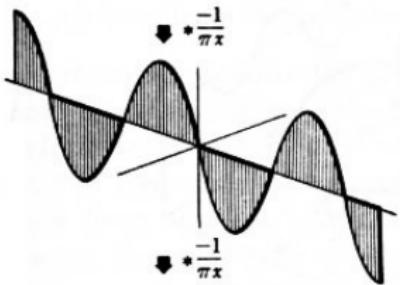
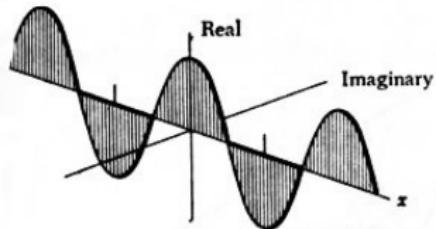
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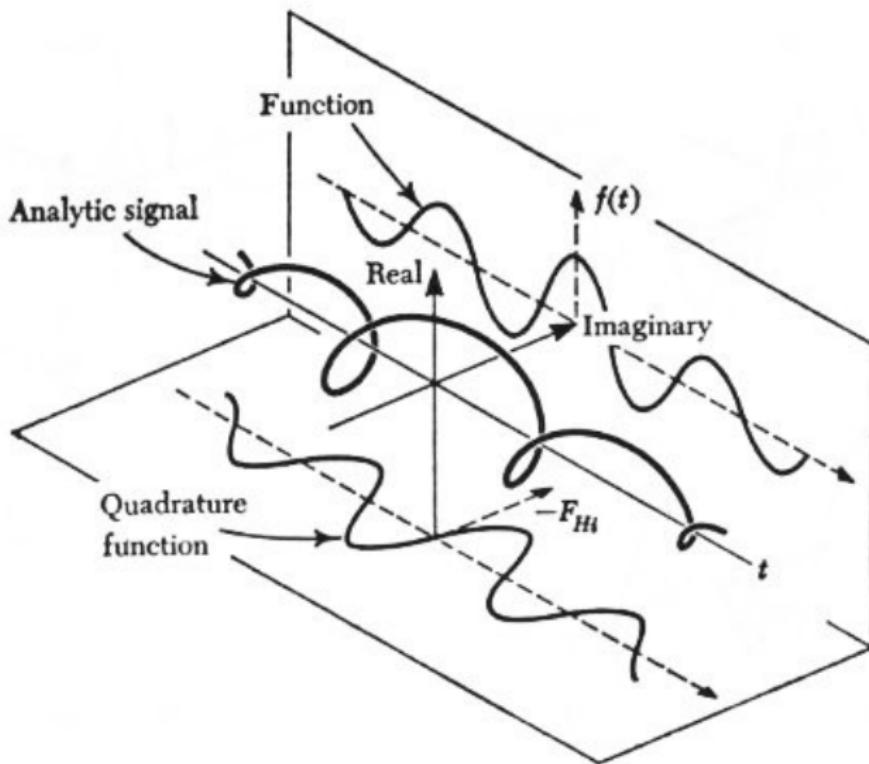
$$e^{i\alpha} = \cos \alpha + i \sin \alpha = \cos \alpha + i \mathcal{H}[\cos \alpha]$$

Let's look at pictures...

Hilbert Transform



The Analytic Signal



Task 2: Index for Phase Synchrony

Basis: how constant is the phase difference over time.

For a review, see Quiroga et al, 2002.

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Example: Mutual Information

Use probability distributions $p(\phi_1)$, $p(\phi_2)$ and $p(\phi_1, \phi_2)$ and calculate the **mutual information**

$$I = \int \int p(\phi_1, \phi_2) \log \frac{p(\phi_1, \phi_2)}{p(\phi_1)p(\phi_2)} d\phi_1 d\phi_2$$

Independence of phases yields $I \approx 0$

Task 2: Index for Phase Synchrony

Basis: how constant is the phase difference over time.

For a review, see Quiroga et al, 2002.

Example: Across Trials

We define the phase locking index

$$PLV(t) = N^{-1} \left| \sum_{n=1}^N \exp(i \Delta\phi(t, n)) \right|$$

where $\Delta\phi(t, n)$ is the phase difference in trial n

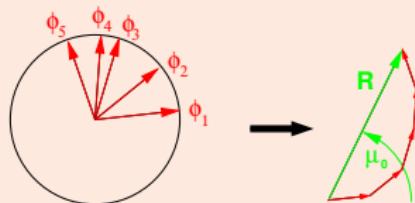
Lachaux et al, 1999

Task 2: Index for Phase Synchrony

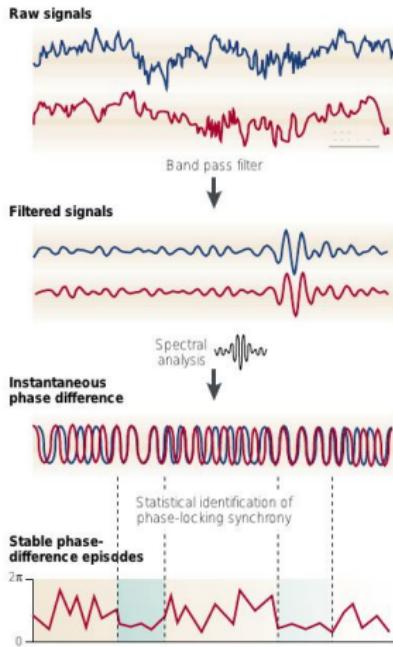
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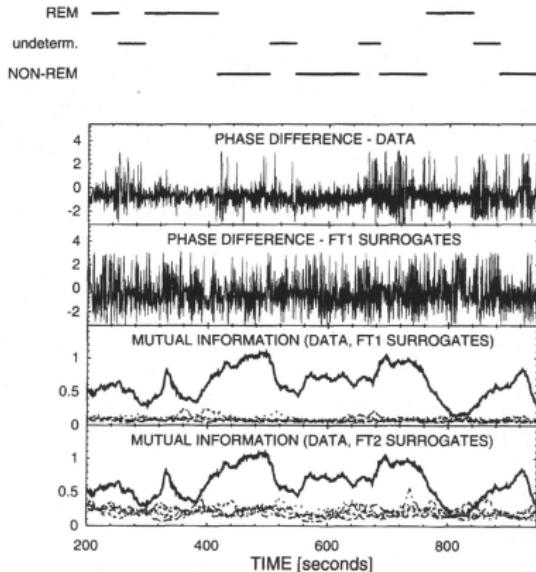
Application to Biology: Phase Synchronization



Varela et al, 2001

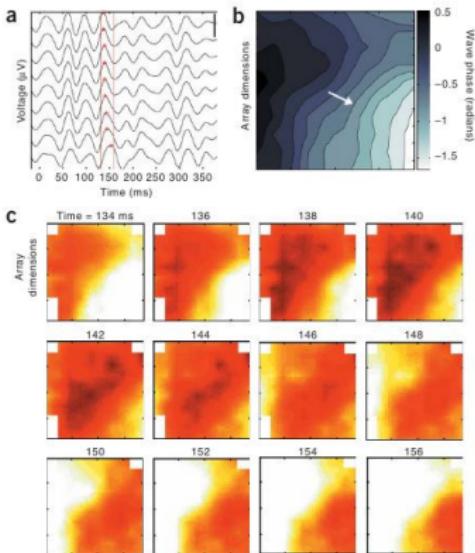
Example: Synchrony in Physiological Measurements

Measurement between respiratory and cardiac signals



Palus, 1997

Example: Measuring LFP wave propagation across cortex



Rubino et al., 2006

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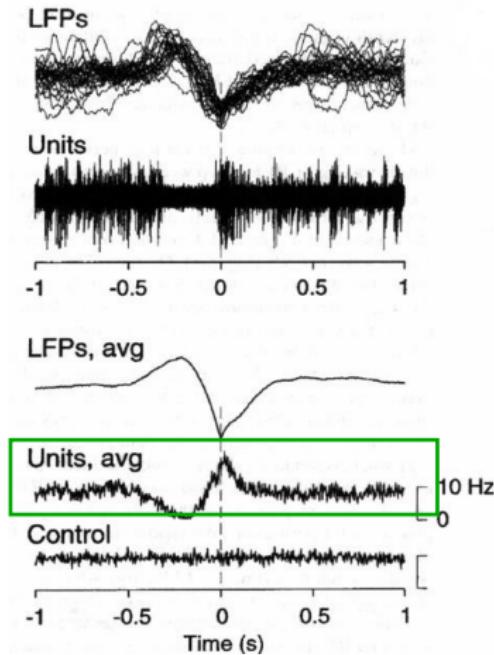
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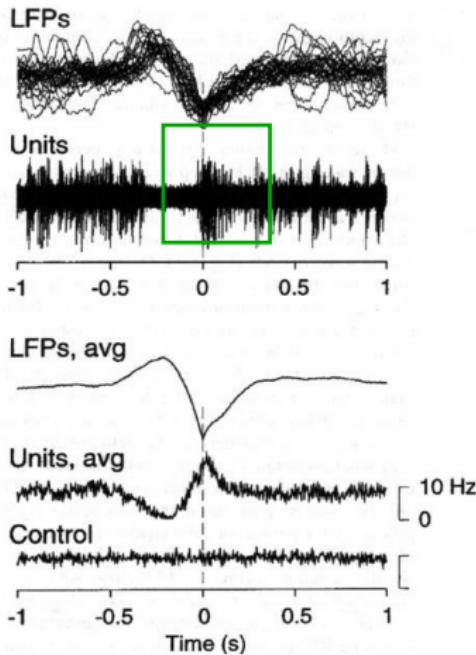
Potential Features of LFP-Spike Relationships



- Locking observed in terms of a **locking probability $p(\phi)$**

Destexhe et al, 1999

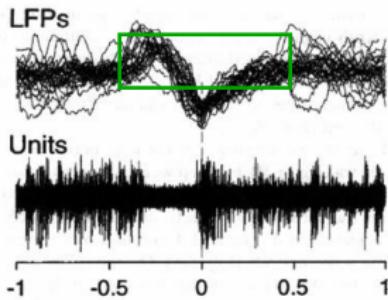
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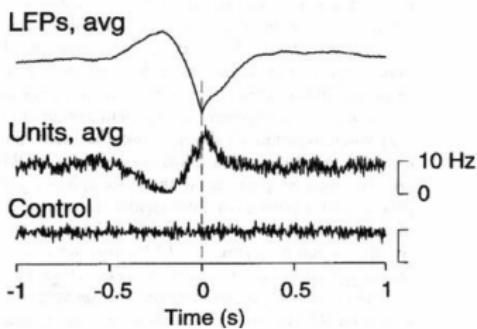
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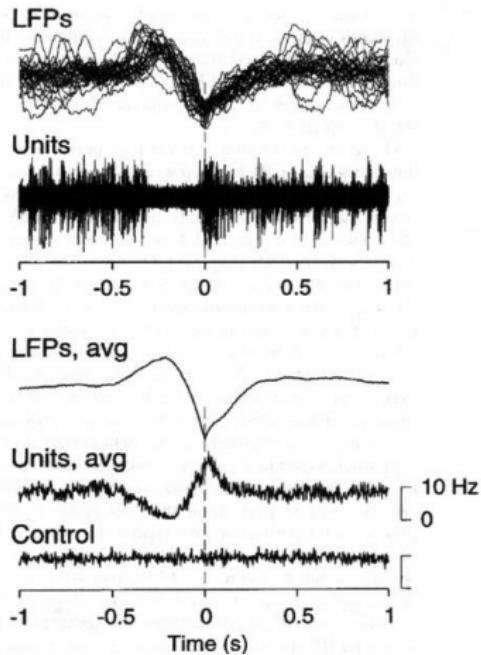


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Destexhe et al, 1999

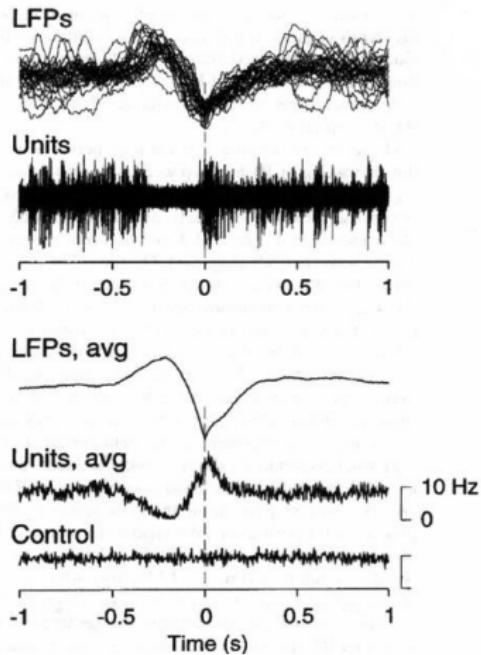
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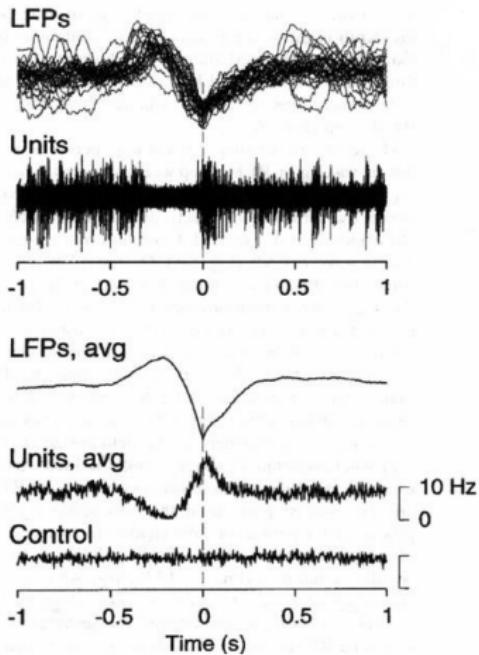
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Destexhe et al, 1999

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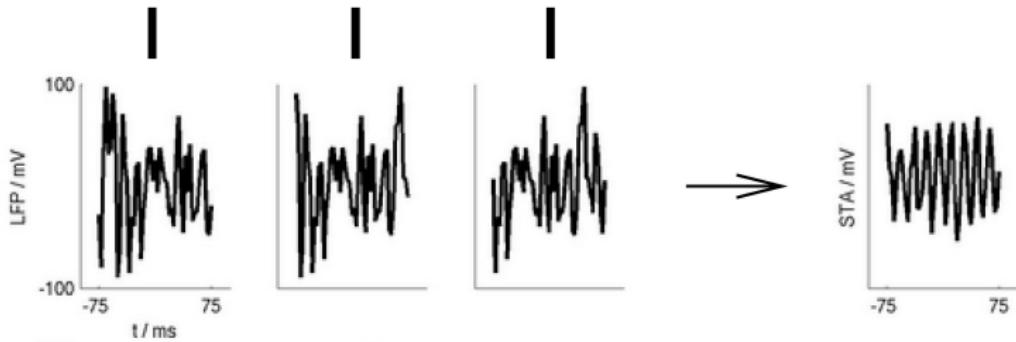
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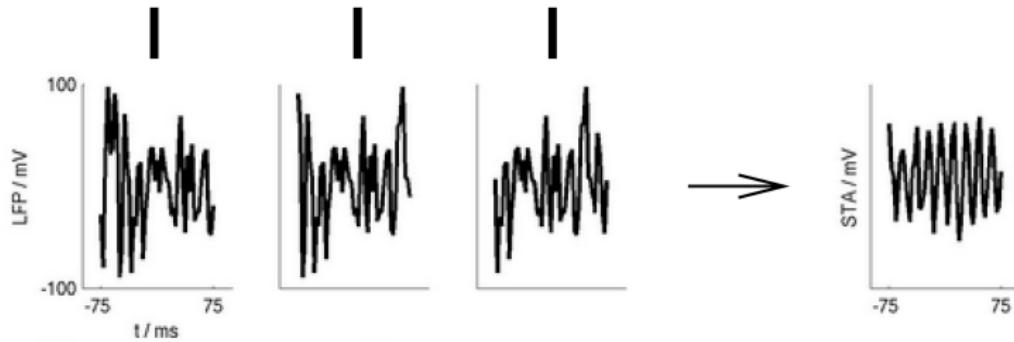
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Spike-Triggered Averaging (STA)



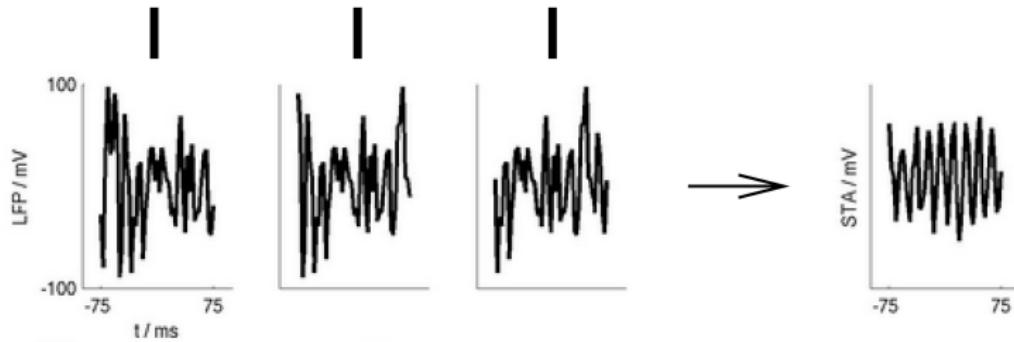
- Cut out LFP segments around spikes...

Spike-Triggered Averaging (STA)



- Cut out LFP segments around spikes...
- ... and average them!

Spike-Triggered Averaging (STA)



- Cut out LFP segments around spikes...
- ... and average them!
- If spikes prefer a specific part of an oscillation cycle, it will not average out in the STA

Spike-Triggered Averaging as Correlation

Assume LFP signal $L(t)$ and a spike train $S(t) = \sum_i \delta(t - t_i)$, where t_i are the spike times

Then, the STA can be written as **correlation** (or alternatively: correlation coefficient)

$$c(\tau) = \int L(t)S(t + \tau) \, dt$$

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However: **Significance** estimate of STA is not trivial.

Typically one uses **surrogates**, such as trial shuffling, shifting the LFP, or bootstrap procedures.

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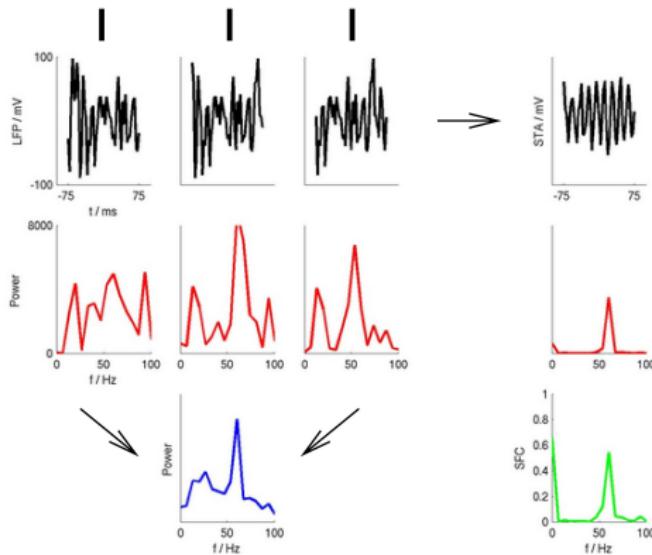
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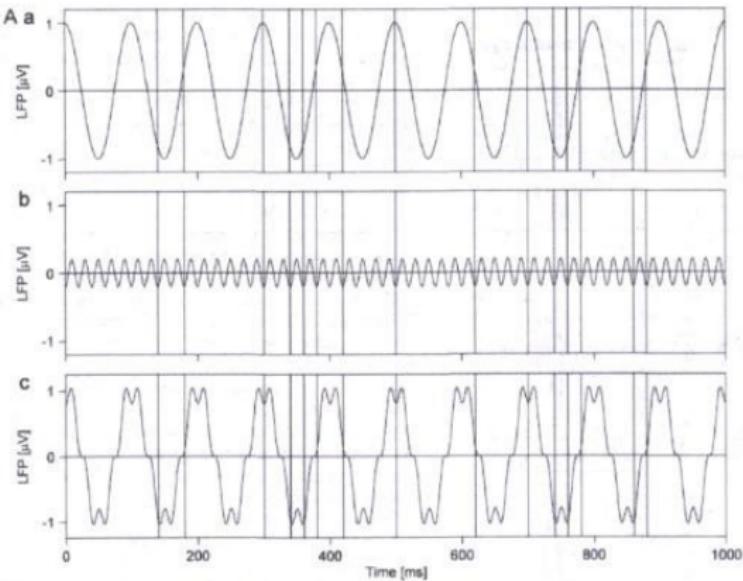
A Simple Spike-Field Coherence (SFC)



SFC is the **power spectrum of the STA**, normalized by average power spectrum of individual segments.

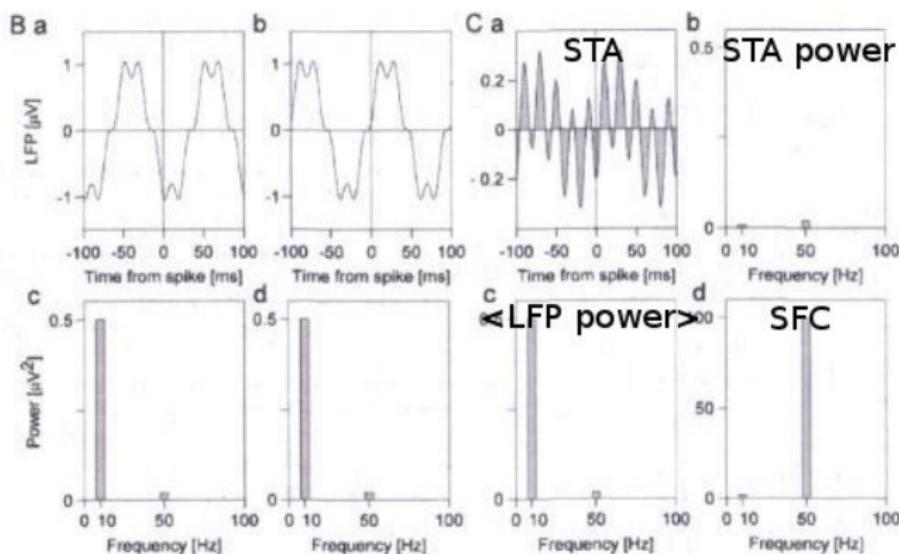
Why the normalization?

Normalization removes mean-amplitude dependence, locking to oscillations with small amplitudes becomes visible



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Insight: Relationship to Coherence

In fact, spike-field coherence is only a **special case** of coherence as discussed before. Why?

for derivations, confidence intervals, see e.g., [Jarvis et al, 2001](#)

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Correlation Theorem (sloppy):

$$\mathcal{F}(CCF(x(t), y(t))) = \mathcal{F}(x(t)) \cdot \mathcal{F}(y(t))$$

where $\mathcal{F}(\cdot)$ denotes the Fourier transform and CCF the cross-correlation function

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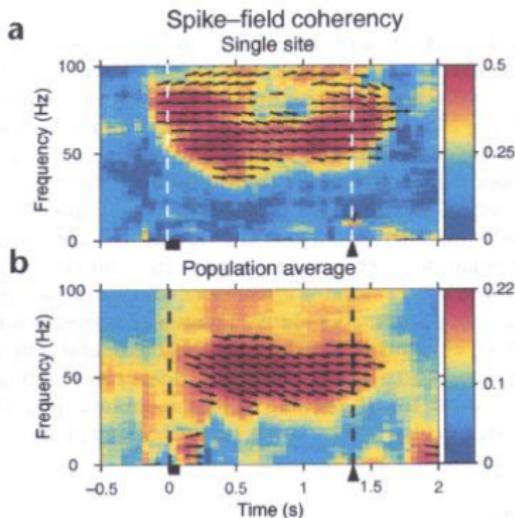
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Previous: STA is the cross correlation of LFP and spike train
Equivalence:

$$\mathcal{F}(STA) = C_{xy}(f)$$

for derivations, confidence intervals, see e.g., [Jarvis et al, 2001](#)

Example: Memory Task in Macaque



Pesaran et al, 2002

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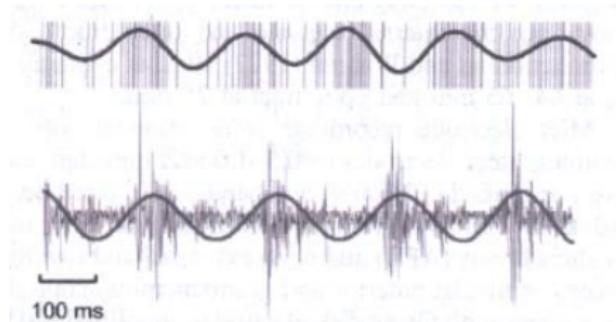
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Extension to Phase Analysis

Simple Idea: Transform spike train to rate signal, and use normal phase synchronization

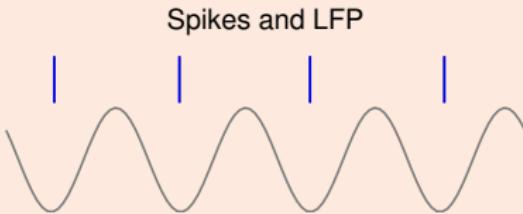


Hurtado et al, 2004

Drawback: Loose precise timing information about spikes
(early average)

E Alternative

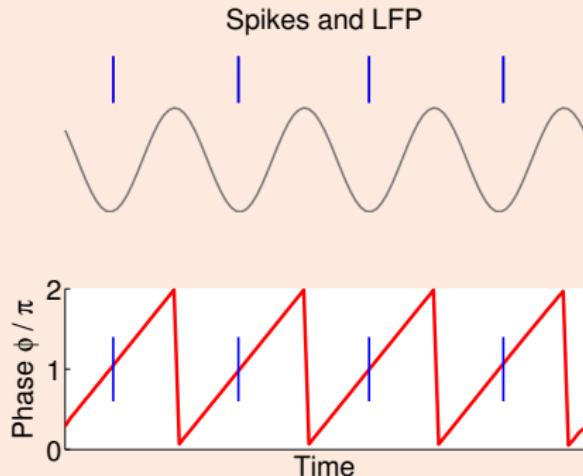
Determine instantaneous **phase** of the LFP signal related to **spike timing**



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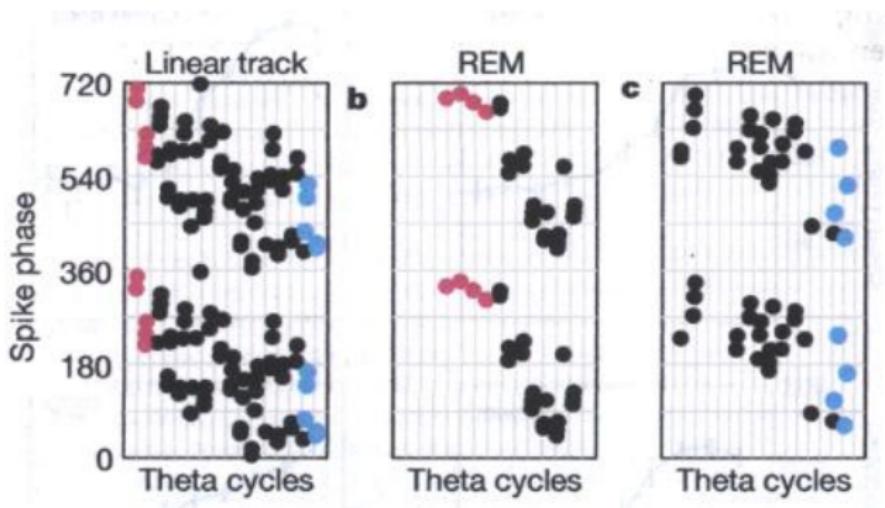


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Direct Phase Estimation

Obtain phases at time instances of discrete occurrences (e.g. spikes)

→ Stroboscopic sampling of the system, a **synchrogram**



Harris et al, 2002

Phase Locking Statistics

Given:

Extracted phases $\phi(t_i)$ of LFP at spike times $t_i, i = 1 \dots N$.

Approach 1: Period Histogram

Bin phase axis $[0; 2\pi)$

Phase Locking Statistics

Given:

Extracted phases $\phi(t_i)$ of LFP at spike times $t_i, i = 1 \dots N$.

Approach 1: Period Histogram

Approach 2: Circular Statistics cf., eg., Mardia and Jupp, 2000

Mean phase μ_0 : $Re^{i\mu_0} = N^{-1} \sum_i e^{i\phi_i}$,

Variance: $S := 1 - R = 1 - N^{-1} \left| \sum_i e^{i\phi_i} \right|^2$,

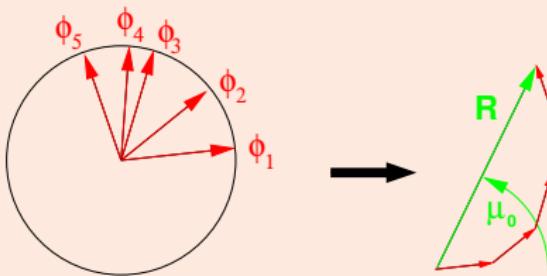
Standard deviation: $\sigma = \sqrt{-2 \ln R}$,

Null hypothesis of uniform phase distribution:

$2NR^2$ is χ^2 -distr. with 2 deg. of freedom.

Phase Locking Statistics

Mean and variance on the circle



Mean phase μ_0 : $Re^{i\mu_0} = N^{-1} \sum_i e^{i\phi_i}$,

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Distribution of R

Approach

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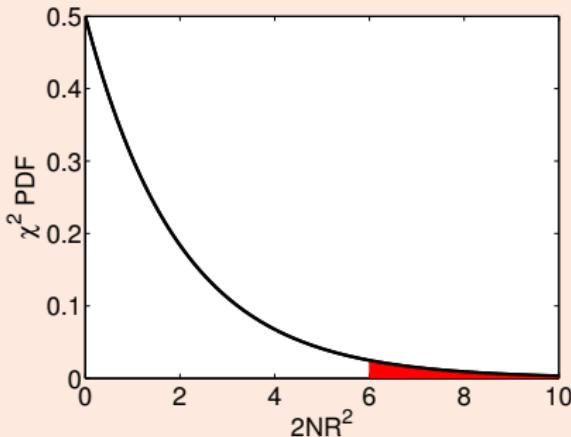
Mean phase

Variance:

Standard

Null hypoth

$2NR^2$ is χ^2



Phase Locking Statistics

Given:

Extracted phases $\phi(t_i)$ of LFP at spike times $t_i, i = 1 \dots N$.

Approach 1: Period Histogram

Approach 2: Circular Statistics cf., eg., Mardia and Jupp, 2000

Mean phase μ_0 : $Re^{i\mu_0} = N^{-1} \sum_i e^{i\phi_i}$,

Variance: $S := 1 - R = 1 - N^{-1} \left| \sum_i e^{i\phi_i} \right|^2$,

Standard deviation: $\sigma = \sqrt{-2 \ln R}$,

Null hypothesis of uniform phase distribution:

$2NR^2$ is χ^2 -distr. with 2 deg. of freedom.

Phase Locking Statistics

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Approach 1: Period Histogram

Approach 2: Circular Statistics

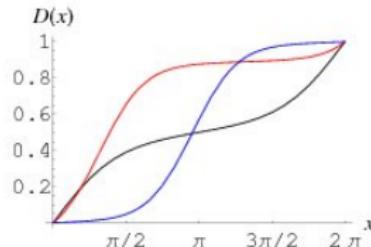
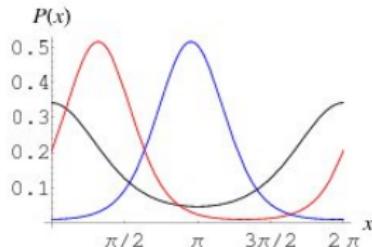
Non-stationarity / Transient Locking

Analysis performed in **sliding windows**.

Circular tests and the von Mises distribution

- Several **tests** in circular statistics are available, equivalent to tests on the line. [Batchelett, 1976; Fisher, 1995](#)
- Use of bootstrap and resampling methods. [Stark and Abeles, 2005](#)
- Standard unimodel distribution is the **von Mise distribution**

$$P_{a,b}(x) = \frac{e^{b \cos(x-a)}}{2\pi I_0(b)}$$



[Weisstein \(MathWorld\)](#)

Using Surrogates To Detect Genuine Locking

- Q: When I observe phase synchronization between two signals, is it **real**?

Using Surrogates To Detect Genuine Locking Synchronization?



Using Surrogates To Detect Genuine Locking

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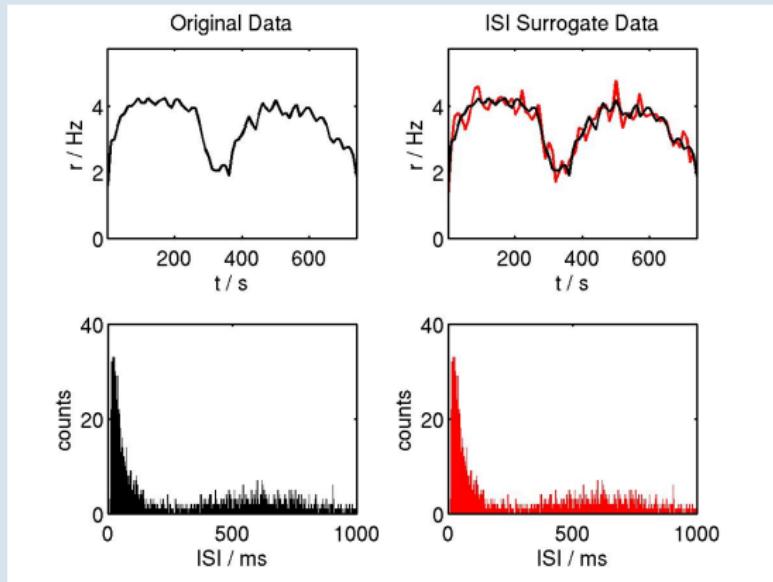
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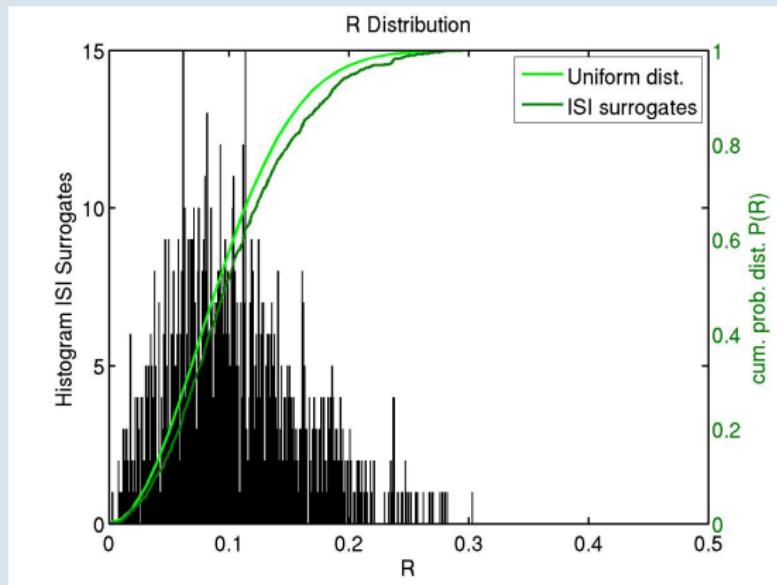
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- Here: Surrogates by **locally** shuffling inter-spike intervals

Using Surrogates To Detect Genuine Looking Local ISI Shuffles



Using Surrogates To Detect Genuine Looking R Distributions



The Meaning of Phase

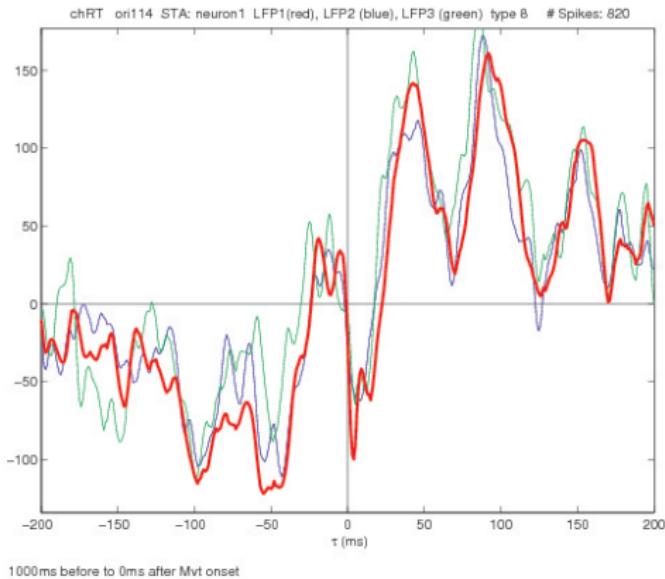
- Instantaneous phase (IP) and Fourier phase (FP) are two distinct measures!
- Interpretation of IP is **controversial**.
- Commonly instantaneous frequency defined as the **instantaneous** change of phase angle.
- Time-average of the IP frequency is related to the average spectral frequency:

$$\langle f_F \rangle_f = \langle f_{IP} \rangle_t$$

- Hard to interpret IP for **multi-component signals** ...
- ... or **small amplitude signals**!
- IP tracks **non-stationarity** of signals in time.
- SFC and phase-locking are two important **complementary** measures.

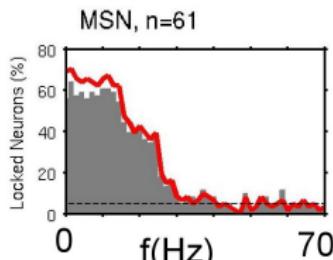
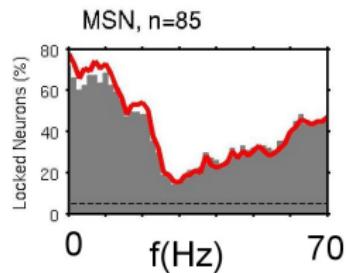
The Electrode Issue

Spikes recorded from the LFP electrode may **contaminate** high frequency LFP



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Today's Exercises

- Task 1: Implement STA and spike-triggered phases
- Task 2: Apply these measures to the data set