# MRE Reconstruction: Inverting the wave equation

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#### Outline of This Talk



- Why we need MRE
- Data Reconstruction and current Problems
- First Experiments
- What comes next



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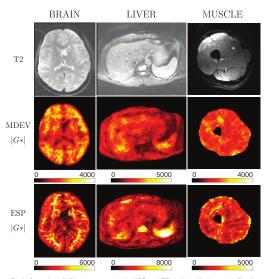


Fig. 9. Comparison of  $|\mathcal{G}|$  and  $\phi$  maps using the MDEV and ESP pipelines. All values are in Pascals.



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 diseased tissue changes mechanical

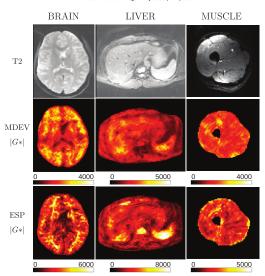


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- ▶ low tech: palpation

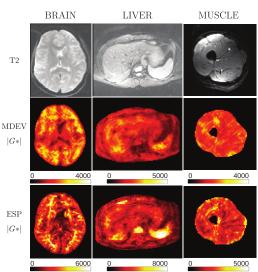


Fig. 9. Comparison of  $|\mathcal{G}'|$  and  $\phi$  maps using the MDEV and ESP pipelines. All values are in Pascals.



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- diseased tissue changes mechanical
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- higher tech: ultrasound

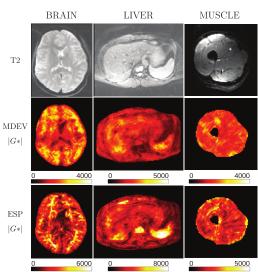


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highest tech: MRE

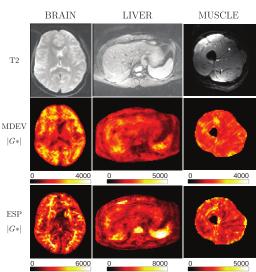


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- diseased tissue changes mechanical
- ▶ low tech: palpation
- higher tech: ultrasound
- highest tech: MRE
- for deep tissue and brains, but non-invasive

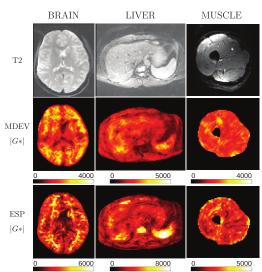
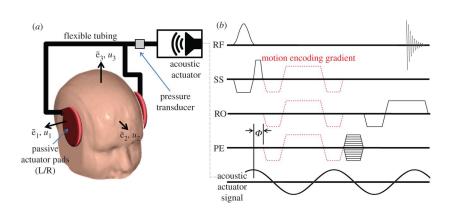


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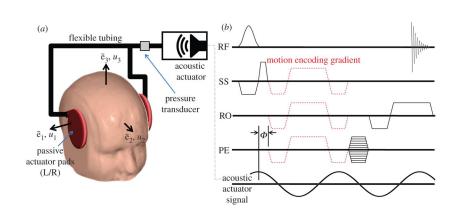
## How does the measuring process work?





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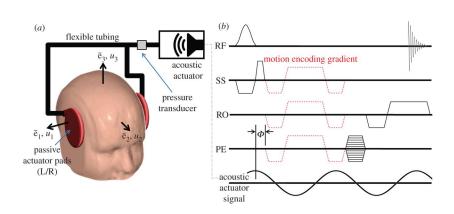




ightharpoonup 3 spatial directions imes 8 time steps imes 3 frequencies

## How does the measuring process work?





- ▶ 3 spatial directions × 8 time steps × 3 frequencies
- ▶ 72 times longer per pixel than MRI





► Navier-Lamé equation:

$$\sum_{i} \partial_{j} \left( \mu \left( \partial_{j} u_{i} + \partial_{i} u_{j} \right) \right) + \partial_{i} \left( \lambda \partial_{j} u_{j} \right) = \rho \ddot{u}_{i}$$



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time harmonic and small bulk wave

$$\nabla(\boldsymbol{\mu} \cdot \boldsymbol{\epsilon}) = -\rho\omega^2 \mathbf{u}$$
 with  $\epsilon_{ij} = \partial_j u_i + \partial_i u_j$ 



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discretize the equation

$$\left[\nabla \cdot \epsilon + \epsilon \nabla\right] \boldsymbol{\mu} = -\rho \omega^2 \mathbf{u}$$



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$$\left[\nabla \cdot \epsilon + \epsilon \nabla\right] \boldsymbol{\mu} = -\rho \omega^2 \mathbf{u}$$

▶ matrix inversion relies on correct knowledge of  $\mathbf{u}'$ , and  $\mathbf{u}''$ → noise can completely screw up the derivatives

# Noisy displacement field



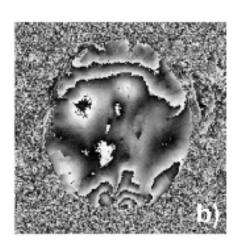


Figure: b) The human brain

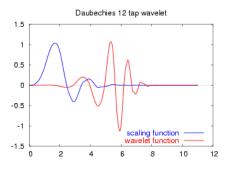




▶  $\mathbf{u}(\mathbf{x},t)$  is piece-wise (very) smooth  $\rightarrow$  sparse in wavelet domain

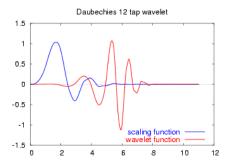


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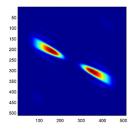


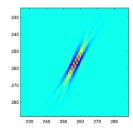
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- ▶ in 2d: anisotropic structure → shearlets





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- ▶ in 2d: anisotropic structure → shearlets





$$\begin{split} u^* &= \underset{u}{\operatorname{argmin}} \ \|u_{\mathsf{meas}} - u\|_2^2 + \lambda \, \|Wu\|_0 \\ &= W^\dagger H \left(Wu_{\mathsf{meas}}; \lambda \right) \end{split}$$

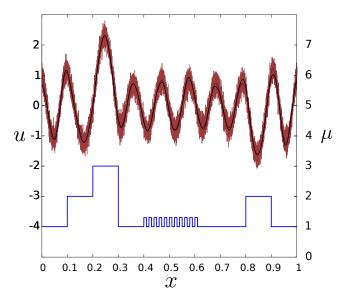


Figure: Shear parameter, displacement and noise in 1d

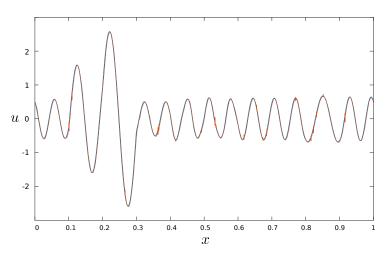


Figure: Reconstructed with Daubeshies10-wavelets and threshold of  $0.01 * \max_i(u_i)$ 

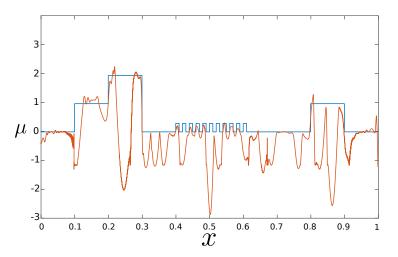


Figure: Original and reconstructed shear parameter  $\mu$ .

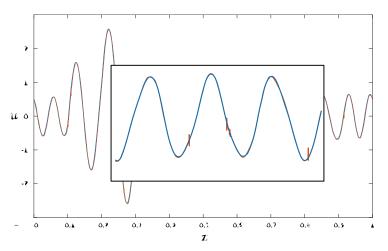


Figure: First derivative of original and denoised displacement u. Close-up reveals noise residuals on a fine scale.

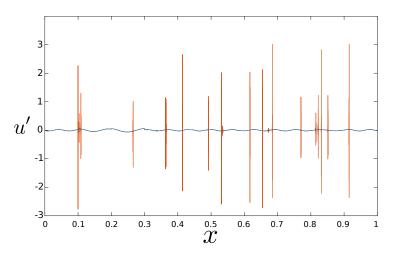


Figure: First derivative of original and denoised displacement u. Fine scale noise dominates the first (and subsequent) derivatives.

## Our plan of work



- Do simuations in 1d: wavelets
- Do simulations in 2d: wavelets, shearlets

- Problem: Need to reconstruct the derivatives
- ▶ slight noise can lead to totally wrong derivatives —¿ inversion is useless
- ▶ MRI measurement in 3 spatial directions and 8 time steps –¿

#### What would be nice results



- Have better resolution of the stiffness map
- Have clinically useful values, at the moment to varying
- Have shorter acquisition times per pixel
- Problem: Need to reconstruct the derivatives
- ▶ slight noise can lead to totally wrong derivatives –¿ inversion is useless
- ▶ MRI measurement in 3 spatial directions and 8 time steps –¿