

MRE Reconstruction: Inverting the wave equation

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BIOQIC Day 2017
Berlin (Germany)
September 23, 2017



- 1 Why we need MRE
- 2 Data Reconstruction and current Problems
- 3 First Experiments
- 4 What comes next

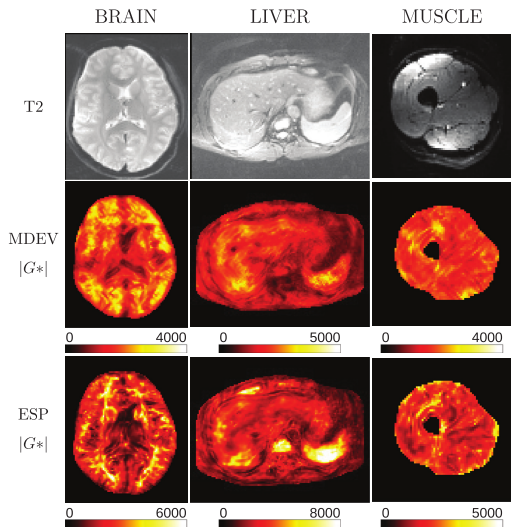


Fig. 9. Comparison of $|G^*|$ and φ maps using the MDEV and ESP pipelines. All values are in Pascals.

- ▶ diseased tissue changes mechanical

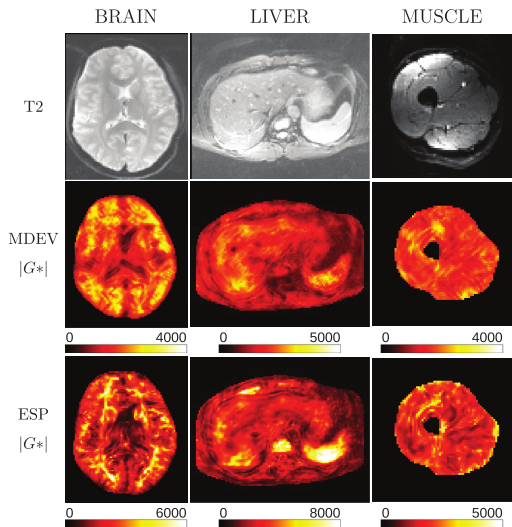


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E. Barnhill et al./Medical Image Analysis 35 (2017) 133–145

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- ▶ low tech: palpation

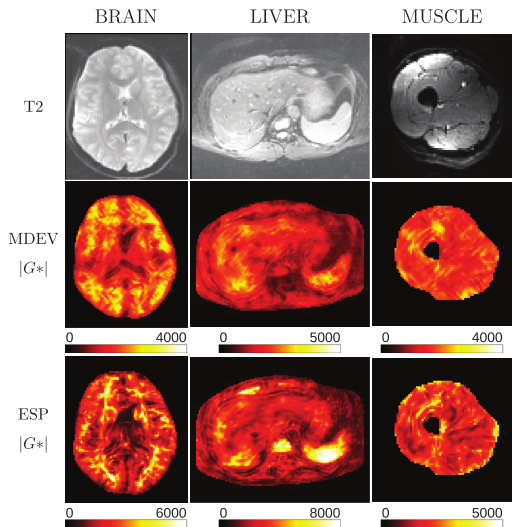


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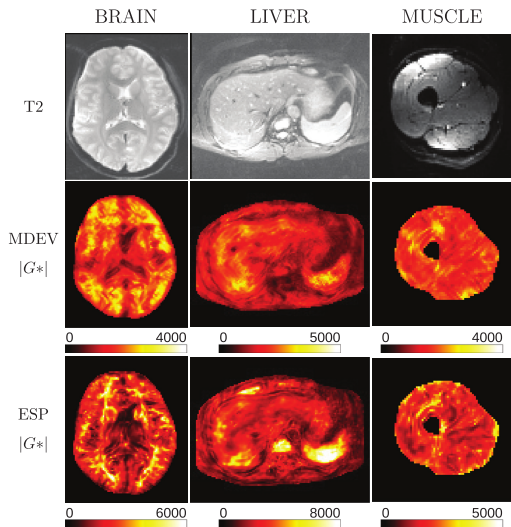


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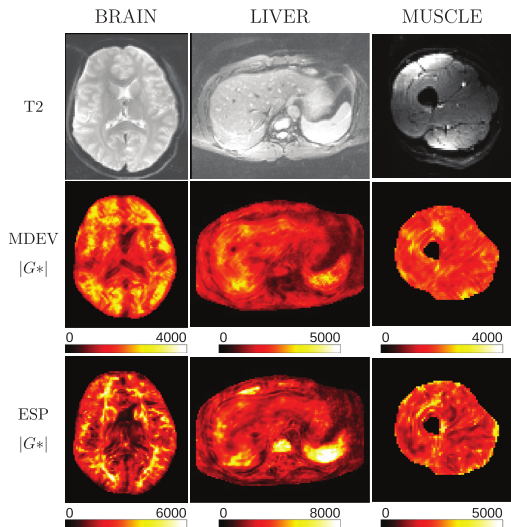


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Why do we need MRE?

- ▶ diseased tissue changes mechanical
- ▶ low tech: palpation
- ▶ higher tech: ultrasound
- ▶ highest tech: MRE
- ▶ for deep tissue and brains, but non-invasive

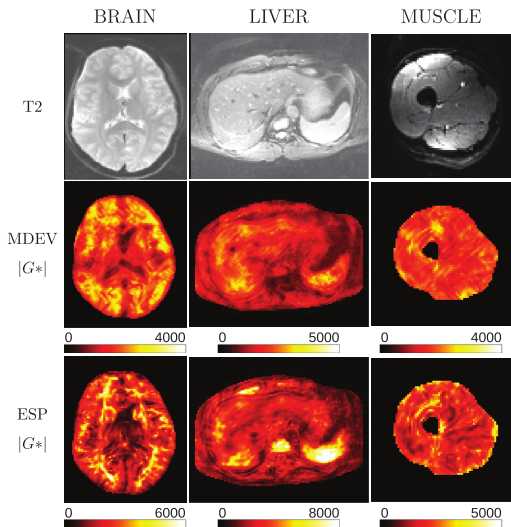
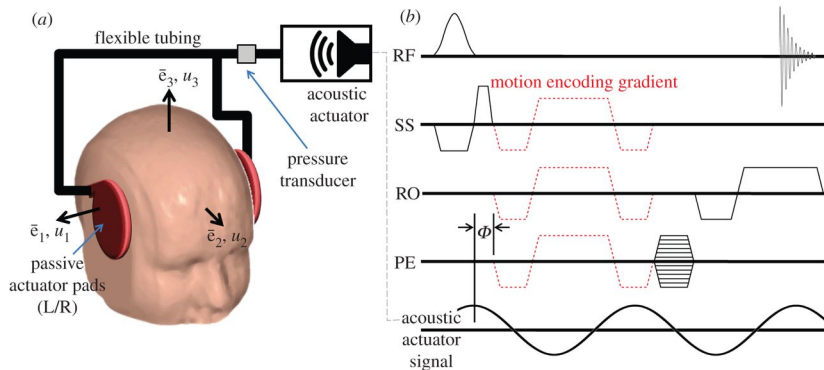
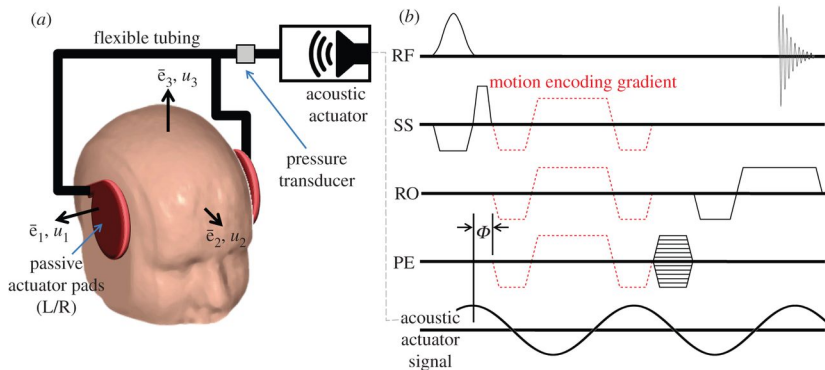


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How does the measuring process work?

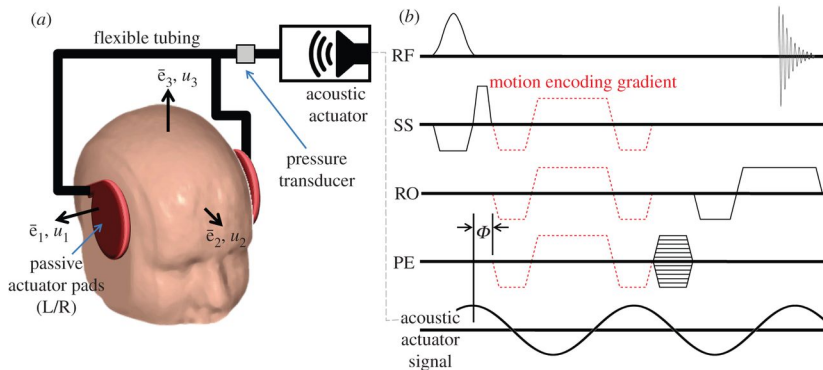


How does the measuring process work?



- ▶ 3 spatial directions \times 8 time steps \times 3 frequencies

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- ▶ 3 spatial directions \times 8 time steps \times 3 frequencies
- ▶ 72 times longer per pixel than MRI

How does the tissue movement relate to stiffness?

- ▶ Navier-Lamé equation:

$$\sum_j \partial_j (\mu (\partial_j u_i + \partial_i u_j)) + \partial_i (\lambda \partial_j u_j) = \rho \ddot{u}_i$$

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- ▶ time harmonic and small bulk wave

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$$[\nabla \cdot \boldsymbol{\epsilon} + \boldsymbol{\epsilon} \nabla] \boldsymbol{\mu} = -\rho \omega^2 \mathbf{u}$$

- ▶ matrix inversion relies on correct knowledge of \mathbf{u}' , and \mathbf{u}''
→ noise can completely screw up the derivatives

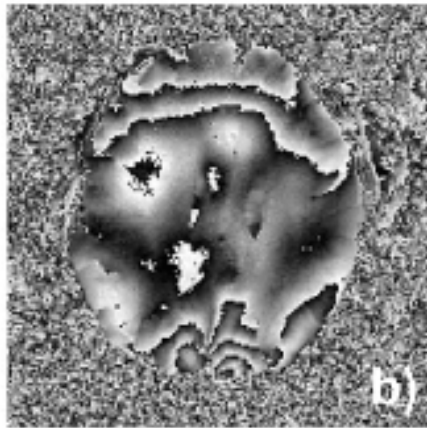
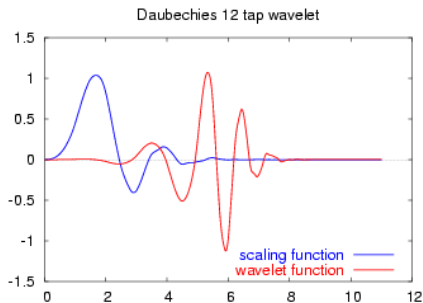


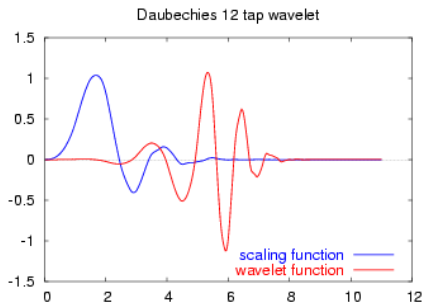
Figure: b) The human brain

- ▶ $\mathbf{u}(\mathbf{x}, t)$ is piece-wise (very) smooth \rightarrow sparse in wavelet domain

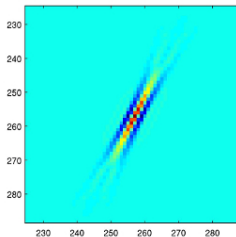
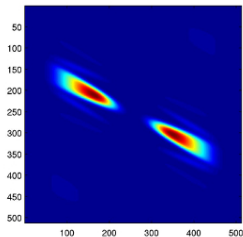
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- ▶ in 2d: anisotropic structure \rightarrow shearlets



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Wavelet Denoising:

$$\begin{aligned} u^* &= \underset{u}{\operatorname{argmin}} \quad \|u_{\text{meas}} - u\|_2^2 + \lambda \|Wu\|_0 \\ &= W^\dagger H(Wu_{\text{meas}}; \lambda) \end{aligned}$$

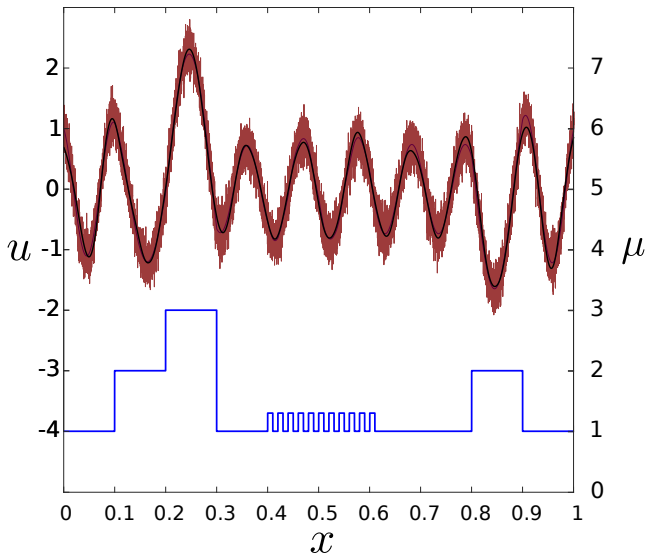


Figure: Shear parameter, displacement and noise in 1d

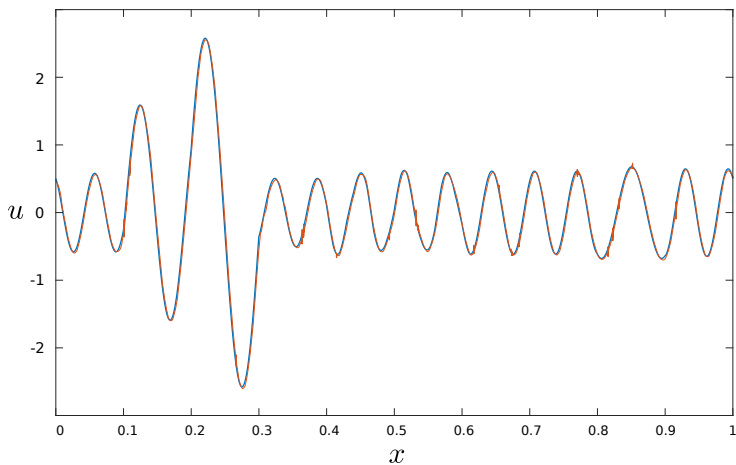


Figure: Reconstructed with Daubeshies10-wavelets and threshold of $0.01 * \max_i(u_i)$

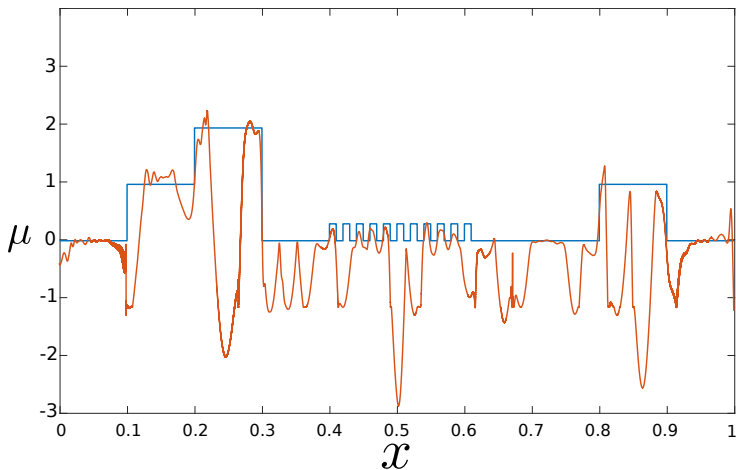


Figure: Original and reconstructed shear parameter μ .

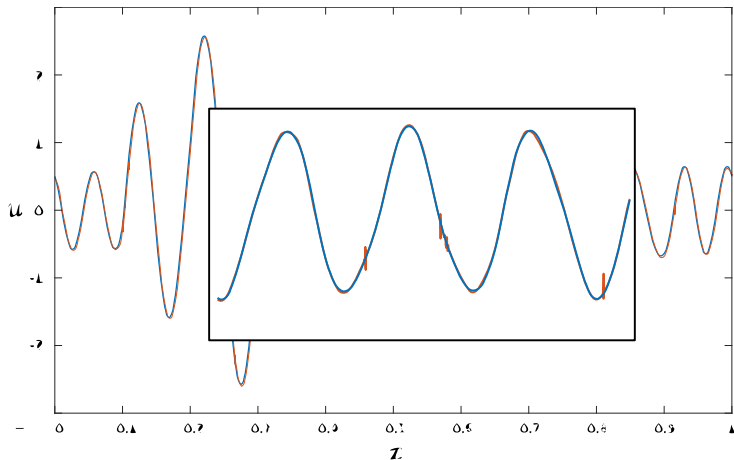


Figure: First derivative of original and denoised displacement u . Close-up reveals noise residuals on a fine scale.

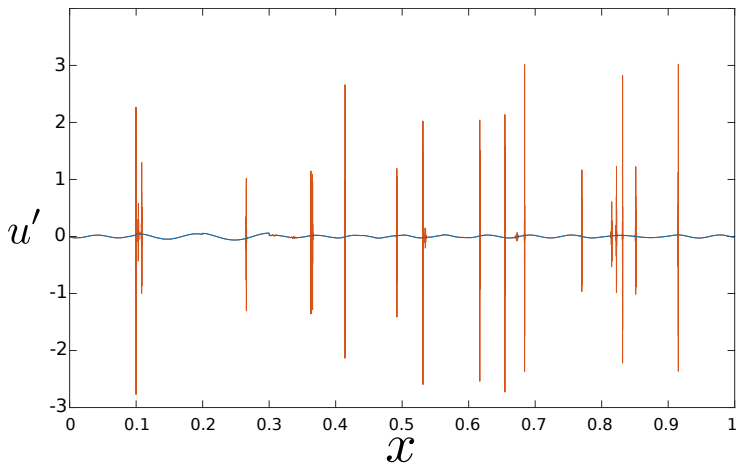


Figure: First derivative of original and denoised displacement u . Fine scale noise dominates the first (and subsequent) derivatives.

- ▶ Do simulations in 1d: wavelets
- ▶ Do simulations in 2d: wavelets, shearlets
- ▶
- ▶ Problem: Need to reconstruct the derivatives
- ▶ slight noise can lead to totally wrong derivatives $-i$ inversion is useless
- ▶ MRI measurement in 3 spatial directions and 8 time steps $-i$

- ▶ Have better resolution of the stiffness map
- ▶ Have clinically useful values, at the moment to varying
- ▶ Have shorter acquisition times per pixel
- ▶ Problem: Need to reconstruct the derivatives
- ▶ slight noise can lead to totally wrong derivatives $-\dot{\chi}$ inversion is useless
- ▶ MRI measurement in 3 spatial directions and 8 time steps $-\dot{\chi}$