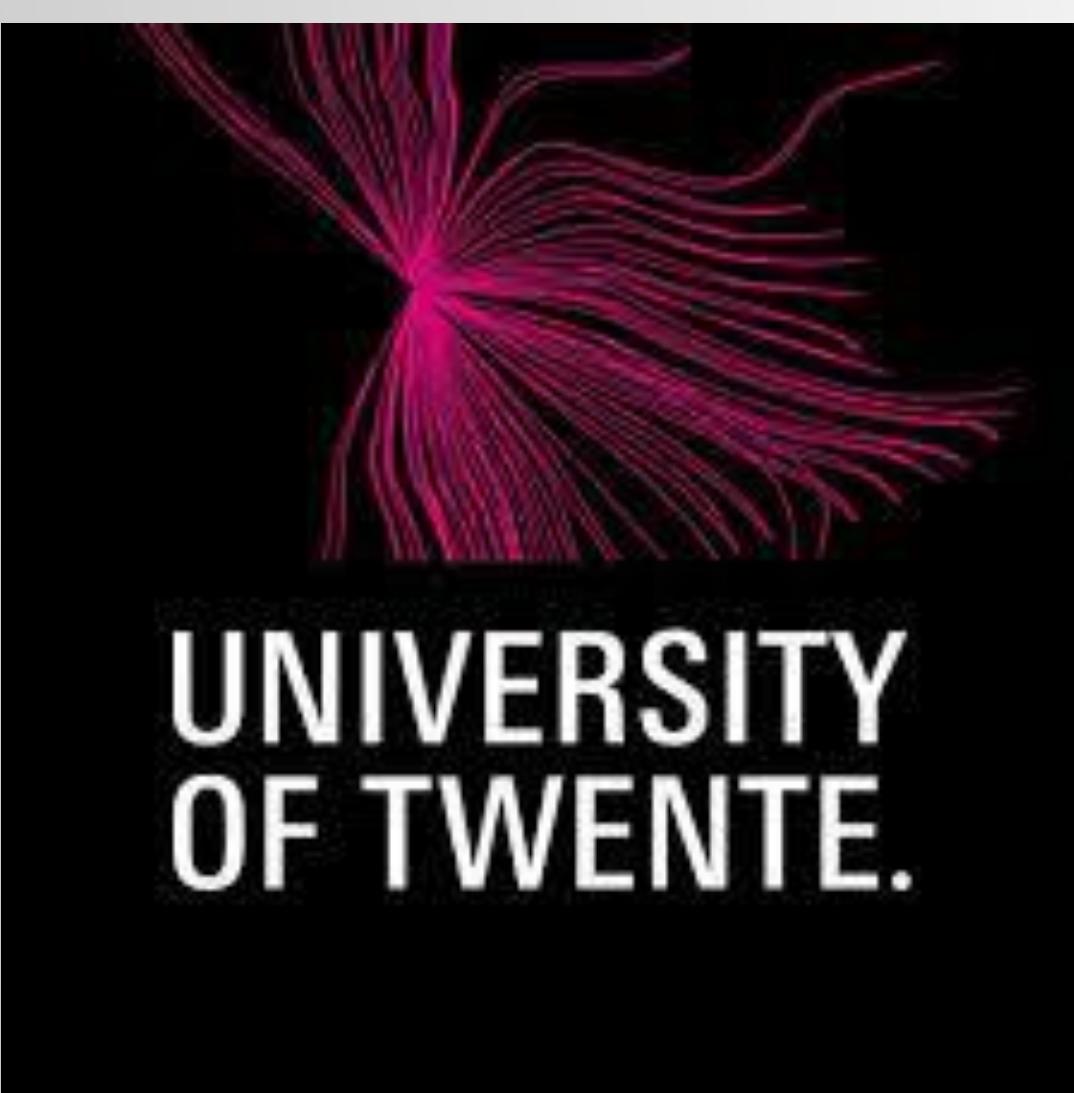


Wearable Coach For Symmetric Walking



Sai Kishan Rali (s2338122)
M.Sc. Embedded Systems

Supervisors

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Prof. Dr. J.S. Rietman
Prof. Dr. J.B.F. Van Erp

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Introduction

- Walking activity + Aging factor
- Person may develop/modify unknowing the way of walking
 - Ideal (symmetric) to abnormal (asymmetric) way of walking
- Treatment
 - Avoiding surgery is not always possible
- After the surgery
 - Kinaesthetic feedback for the joints is affected
- Re-learn the same motor skills (walking). Re-learning
 - Physiotherapists role
 - Supervision of motor re-learning of walking
 - Patients role
 - Attending physiotherapy sessions
 - Home exercises



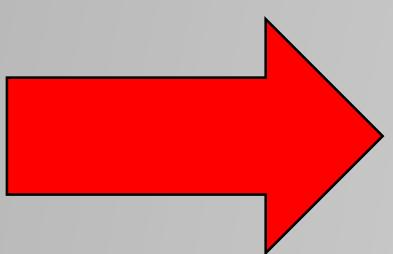
Introduction

- Wearable technology
 - Capable to measure the walking gait
 - Accelerometer
 - Gyroscope
 - Low cost
 - Real-time detection
 - Portable
 - Standalone operation
- Feedback
 - Wearables can also provide feedback
 - Concurrent feedback
- Demonstrates significant therapeutic advantages



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Goal

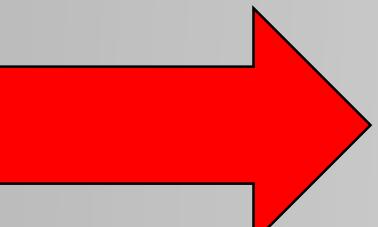
Develop a prototype of a wearable device that provides necessary feedback to the user in real-time which assists in re-learning the right kinaesthetic feedback to the prosthetic joints for symmetrical walking

Research Question

How to design a wearable device that gives haptic feedback for motor learning of patients who undergo hip/knee prosthesis?

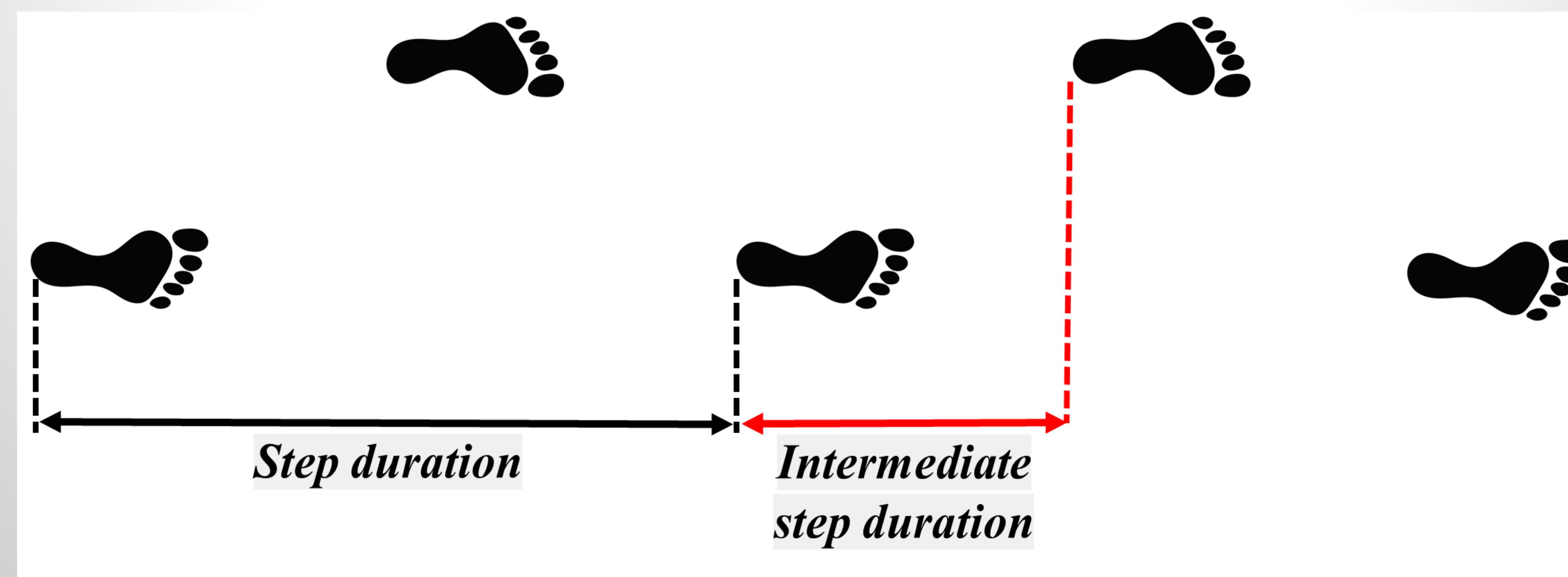
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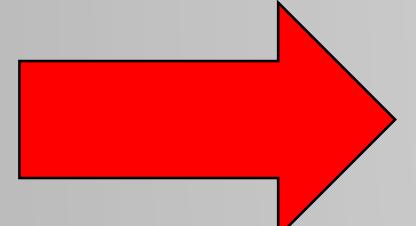


Literature reading conclusions

- **Hypothesis:**
 - The intermediate step duration differs significantly for the users with a prosthesis in the hip/leg in comparison to the users without a prosthesis
 - Sensors positioned on lower back is a good starting points
- Lower back/hips location for providing feedback looks promising
 - Matches with the physiotherapists feedback location
- Feedback strategy leaves more room for experimentation



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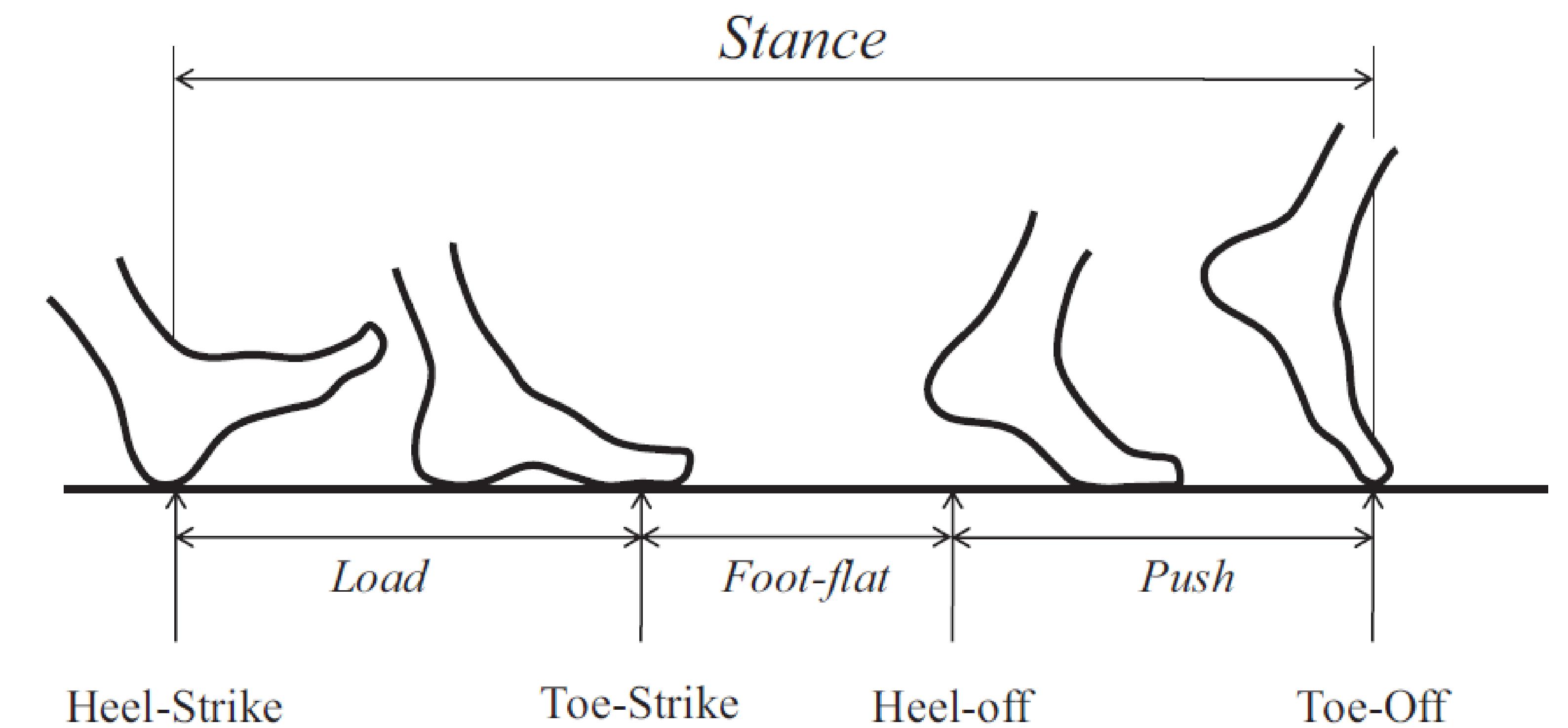
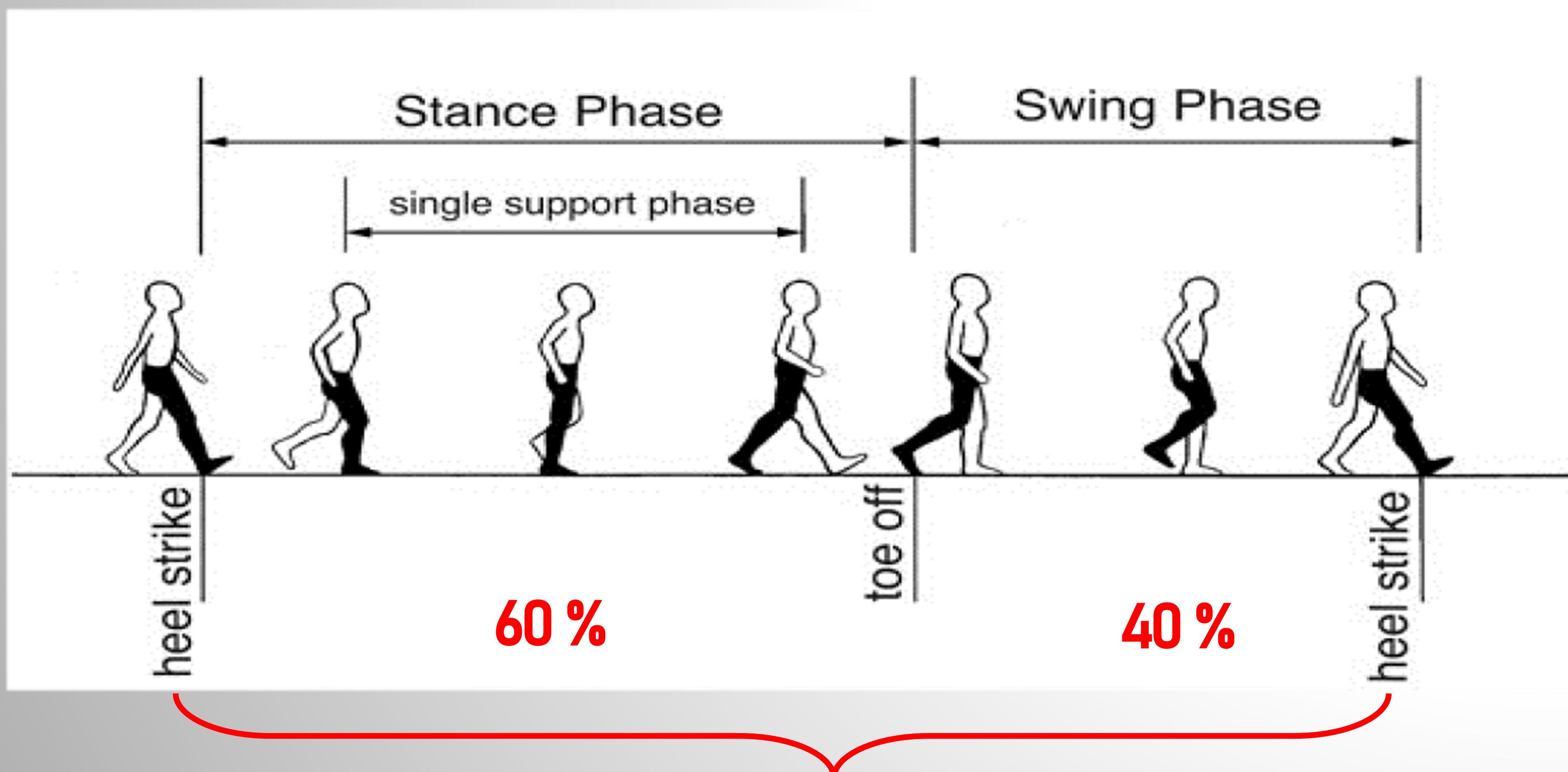
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Pre-Study

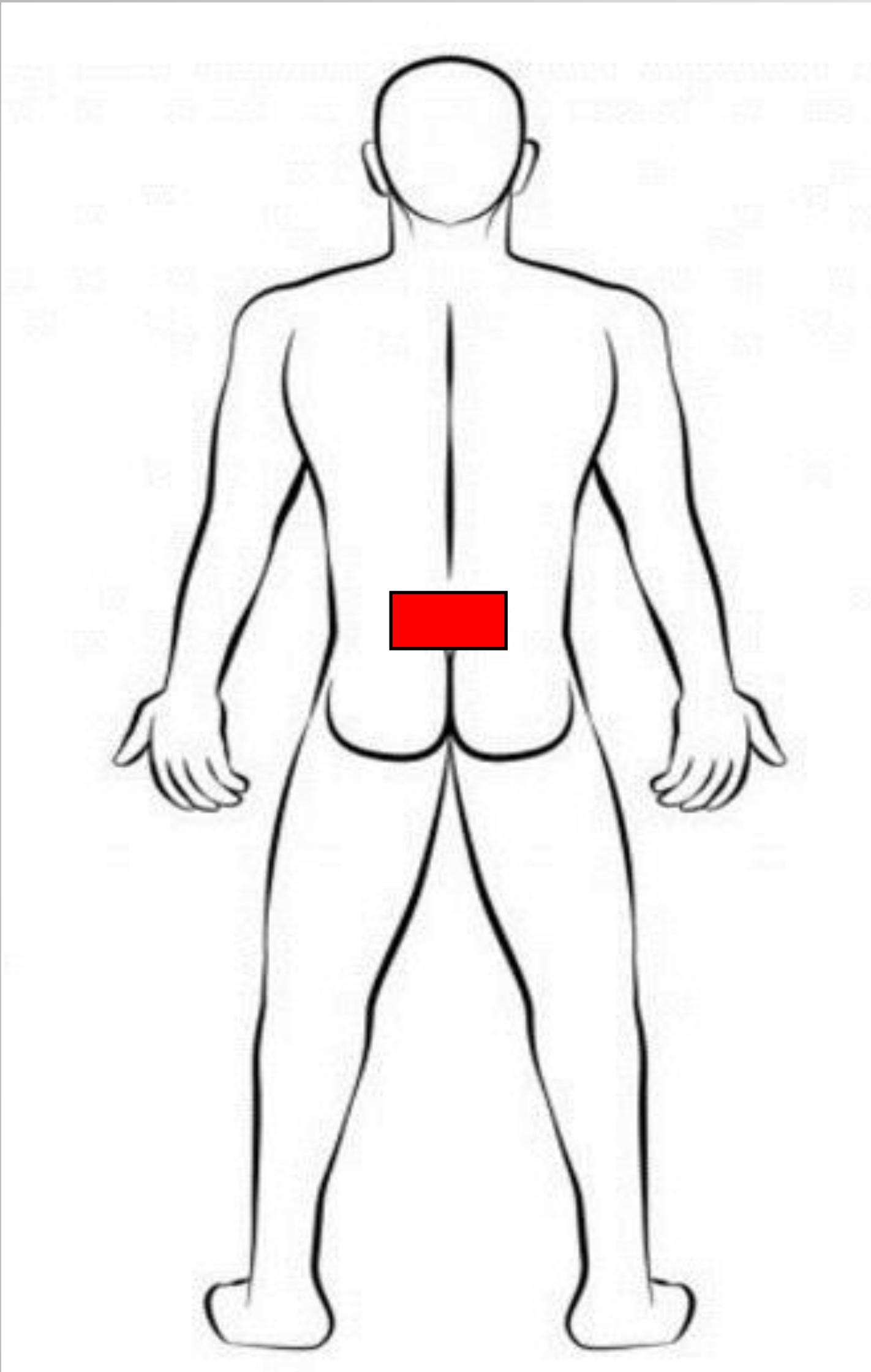
- First development
 - Designing a device to record the IMU measurements
 - Obtaining walking patterns and understanding them for users without prosthesis
- Second development
 - Upgrading the device to match the wearable design requirements
 - Obtaining walking patterns and understanding them for users with prosthesis

Biomechanics of walking

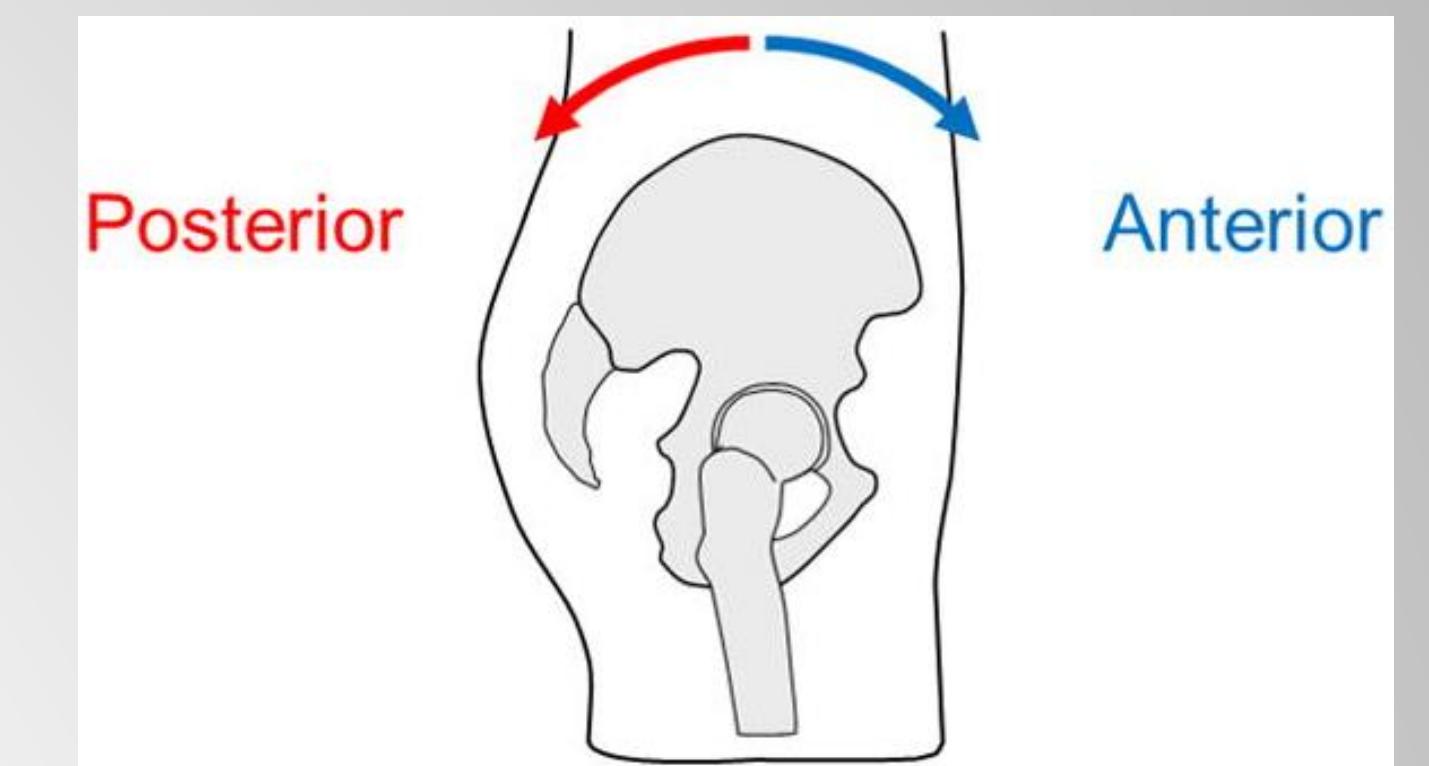
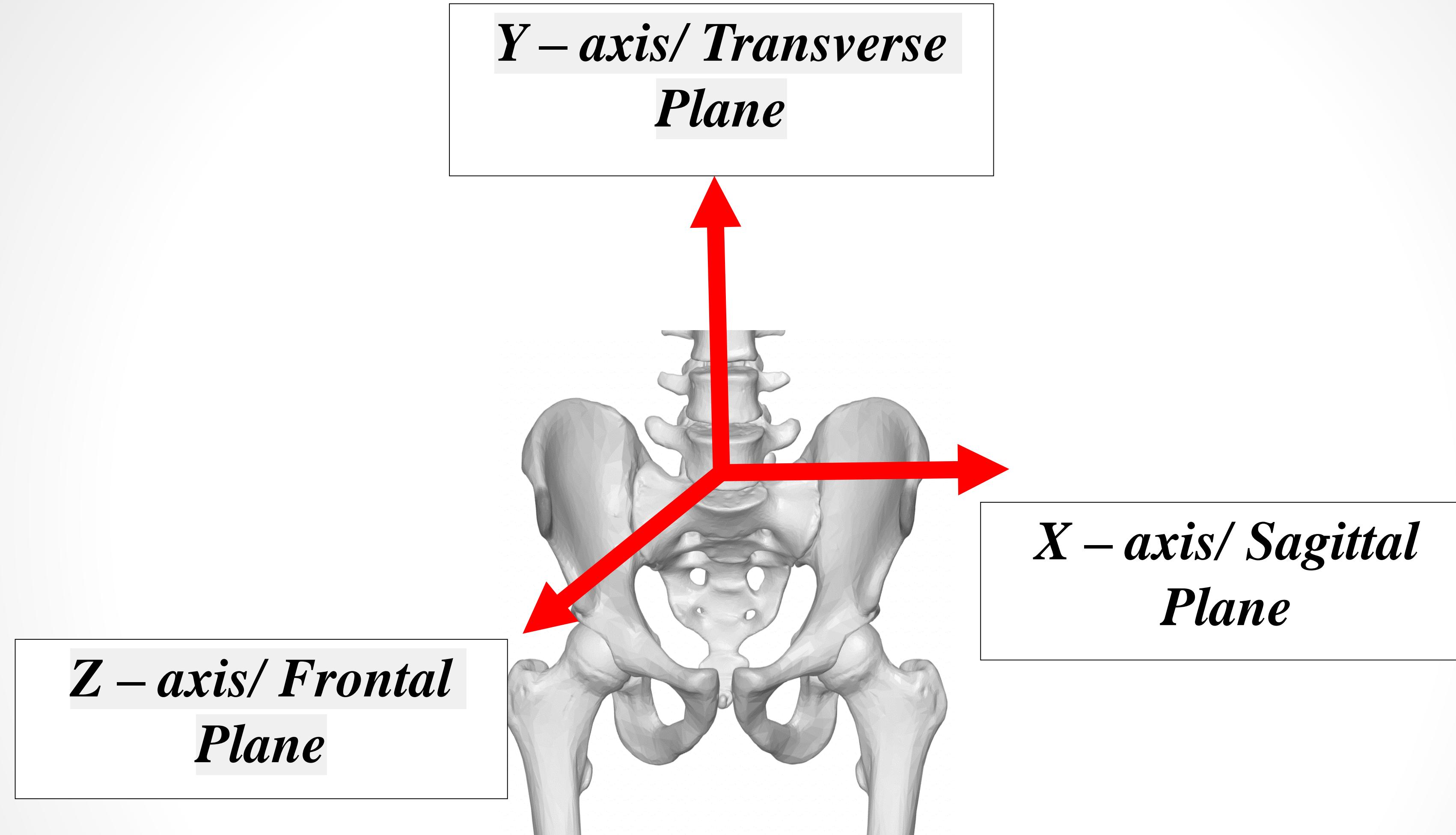
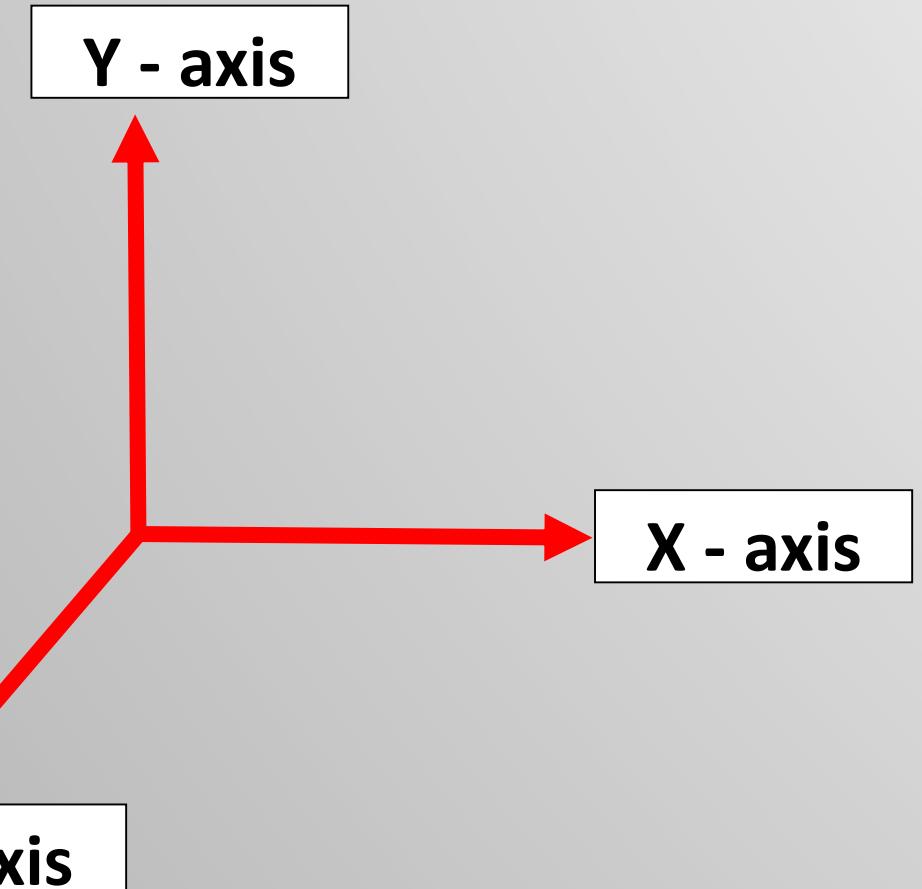
- Walking activity
 - Stance phase
 - Swing phase
- One complete cycle
 - Stance phase + swing phase
($\approx 1 \text{ sec to } 1.2 \text{ sec}$)
- Key events in stance phase
 - Heel-strike
 - Toe-strike
 - Heel-off
 - Toe-off



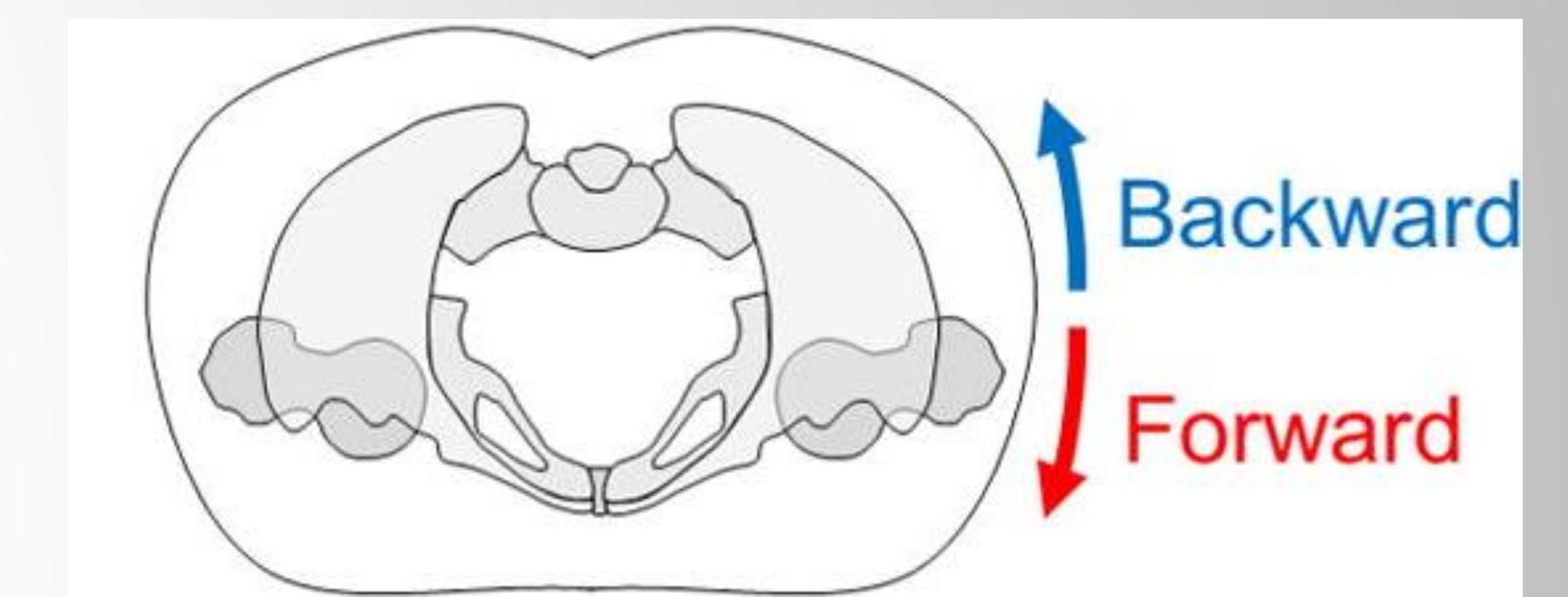
Sensor Location



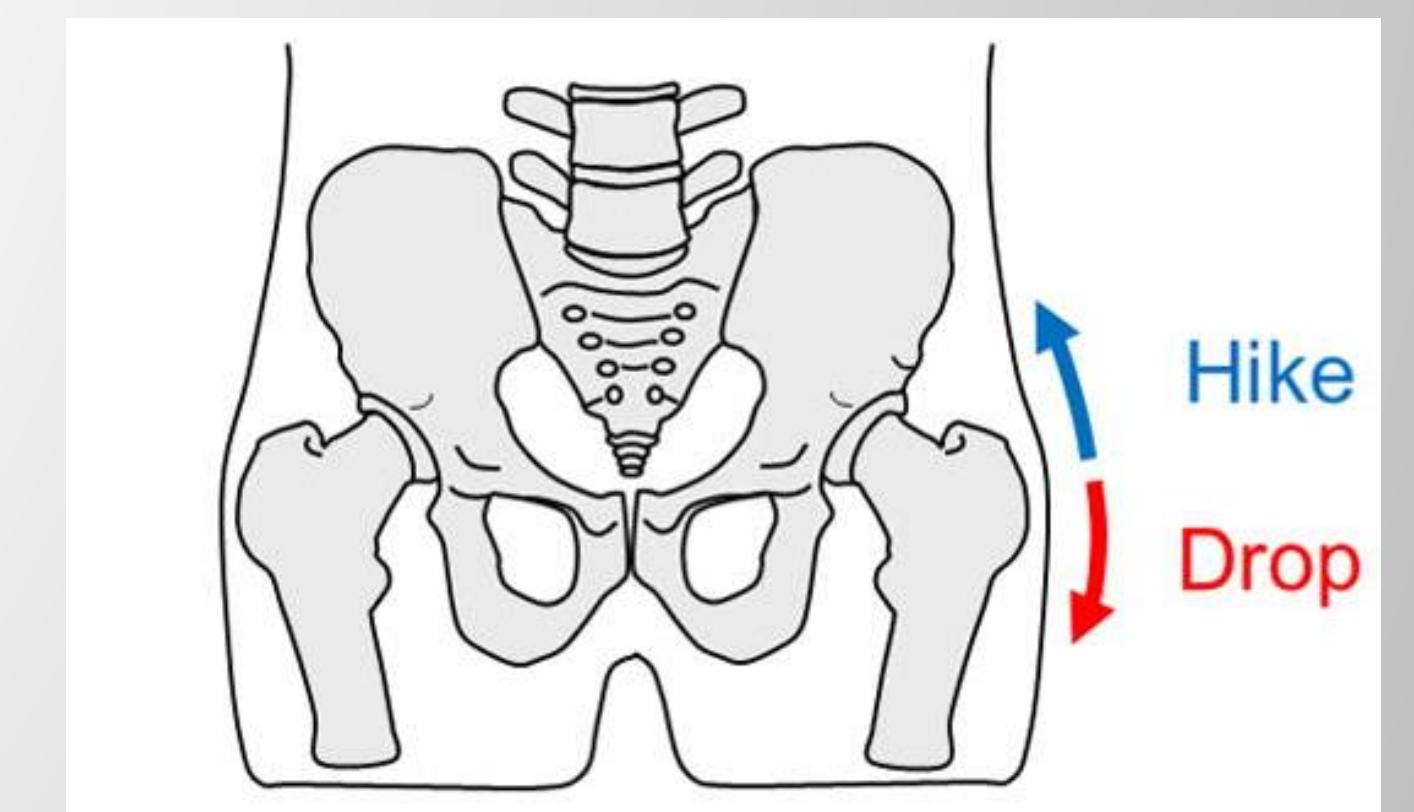
Lower Back



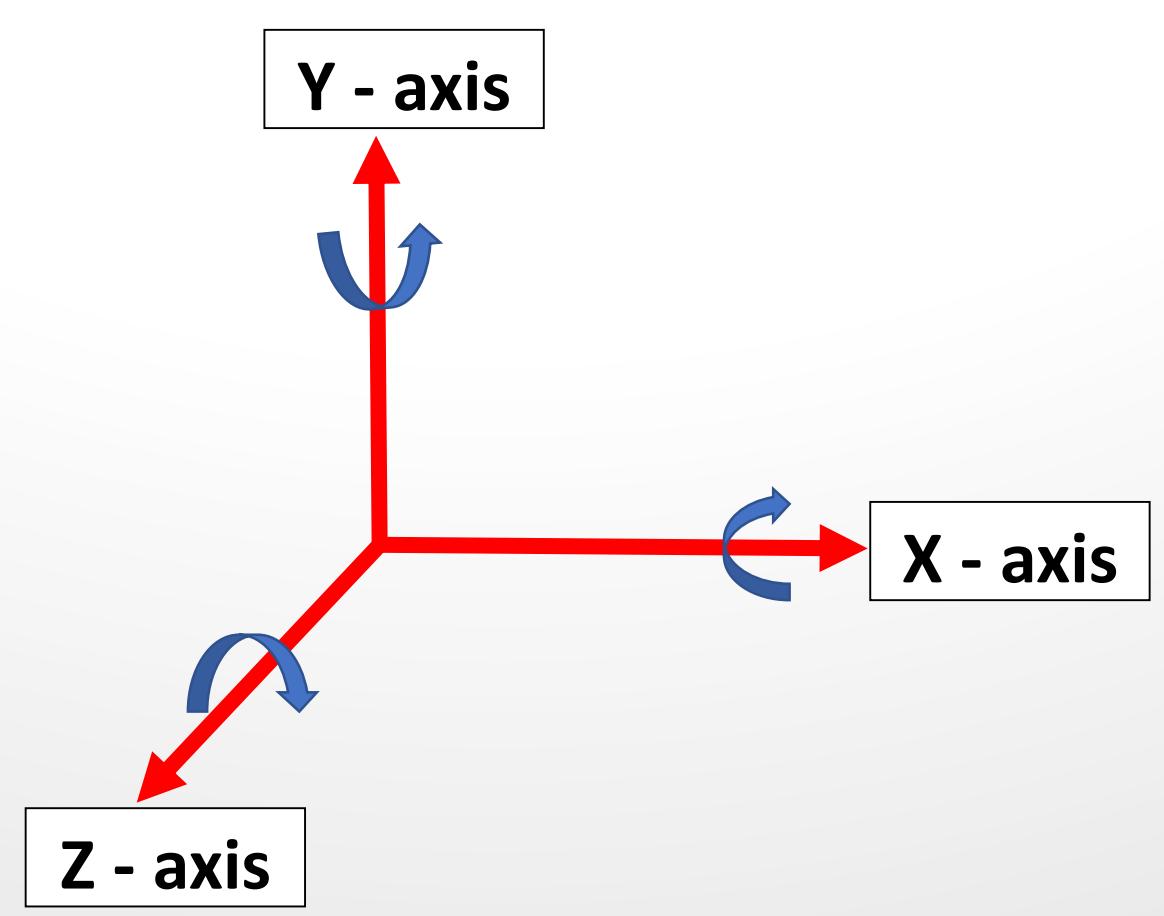
X – axis/ Sagittal Plane



Y – axis/ Transverse Plane

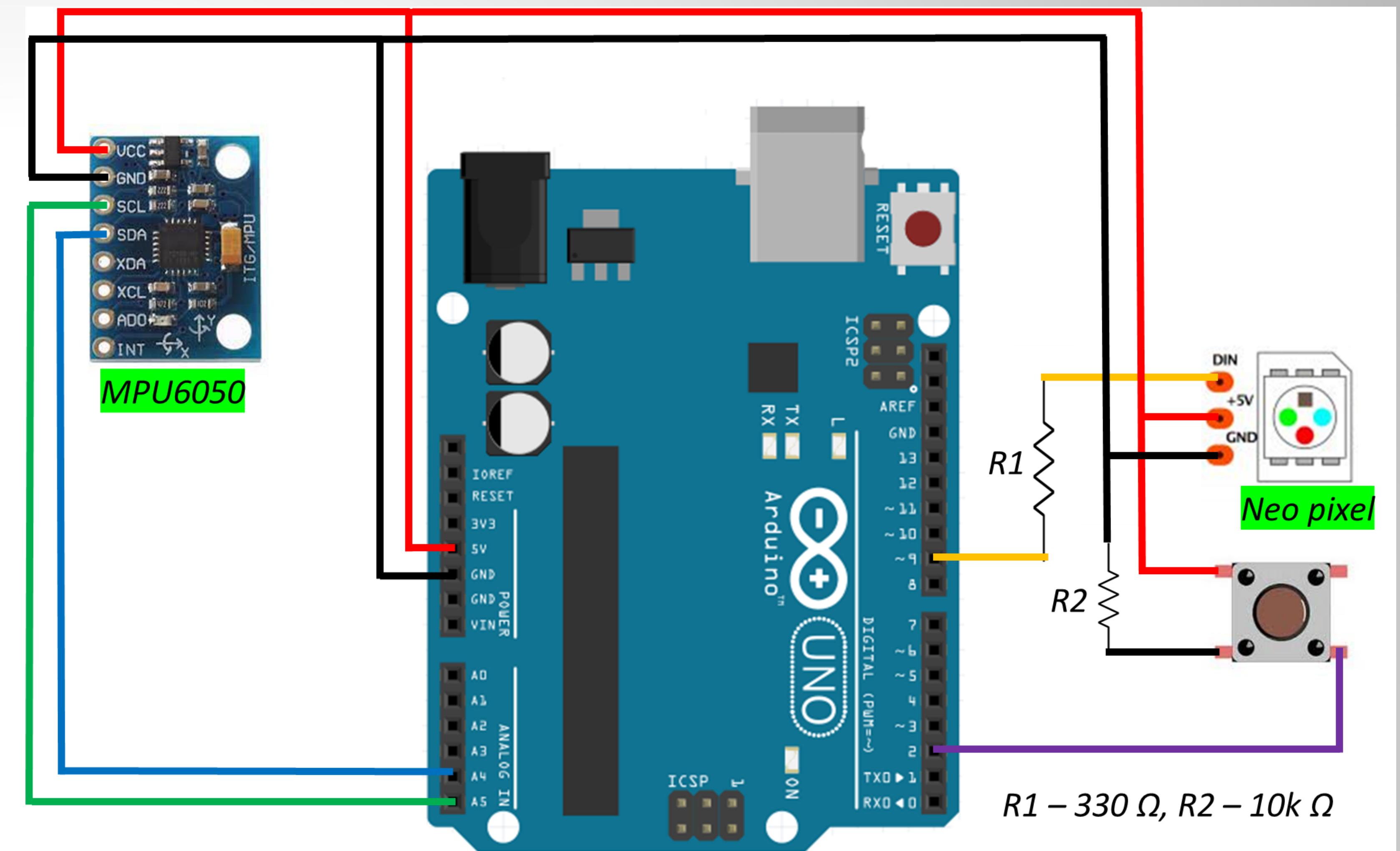


Z – axis/ Frontal Plane



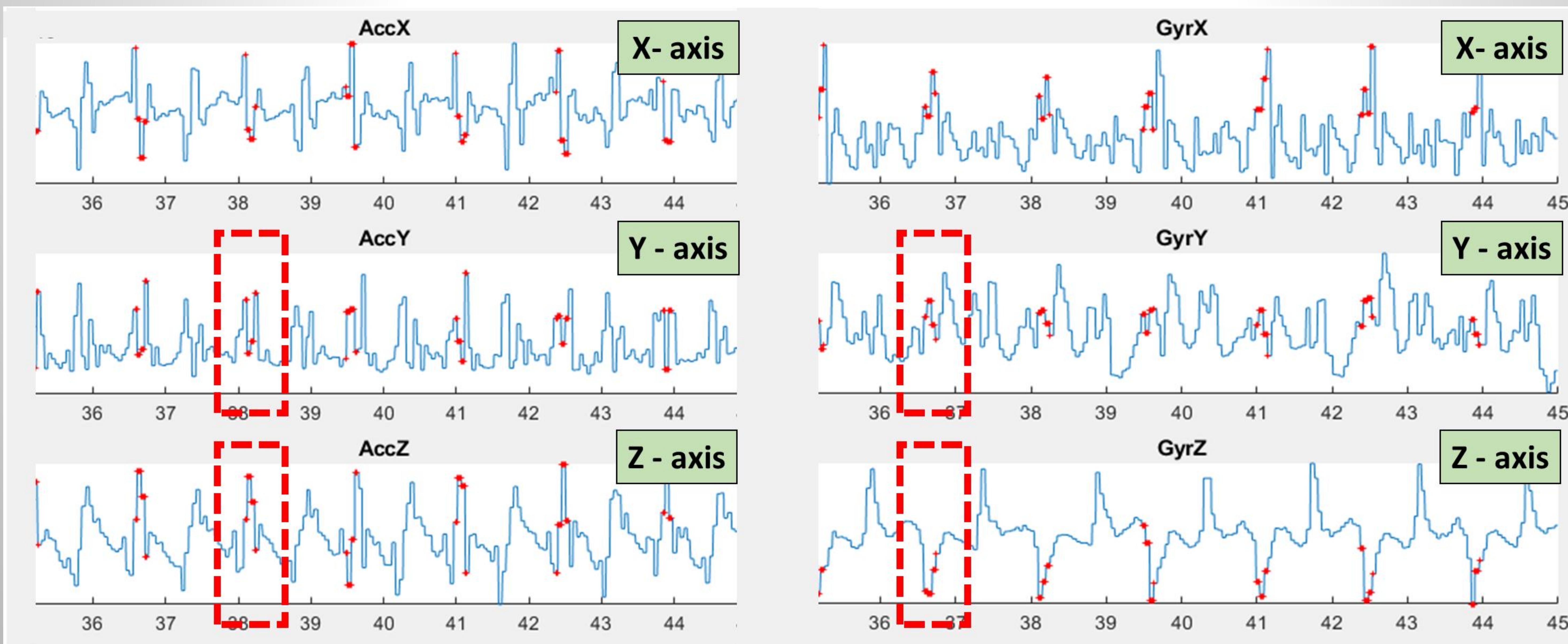
First Development

- Designed wearable device
 - MPU6050 sensor
 - Arduino
 - LED – Neo pixel
 - Button
 - Pouch



First Development

- Observed walking patterns for a user without prosthesis
- Peaks recorded during heel-strike looked promising to develop a real-time algorithm



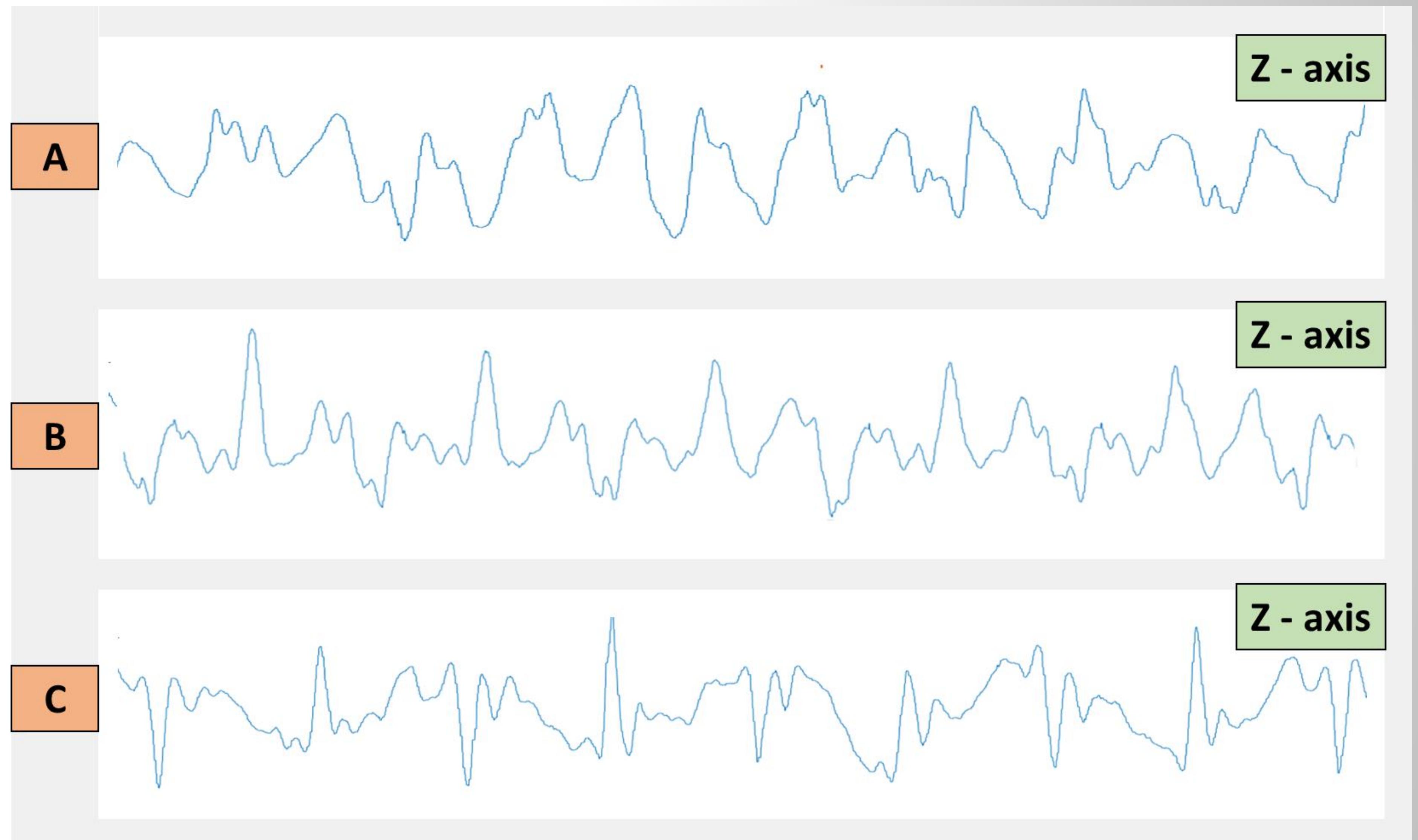
First Development

- When repeated with multiple users
- Measurements along accelerometer Y-axis and Z-axis showcased similar patterns/peaks for the heel-strike event



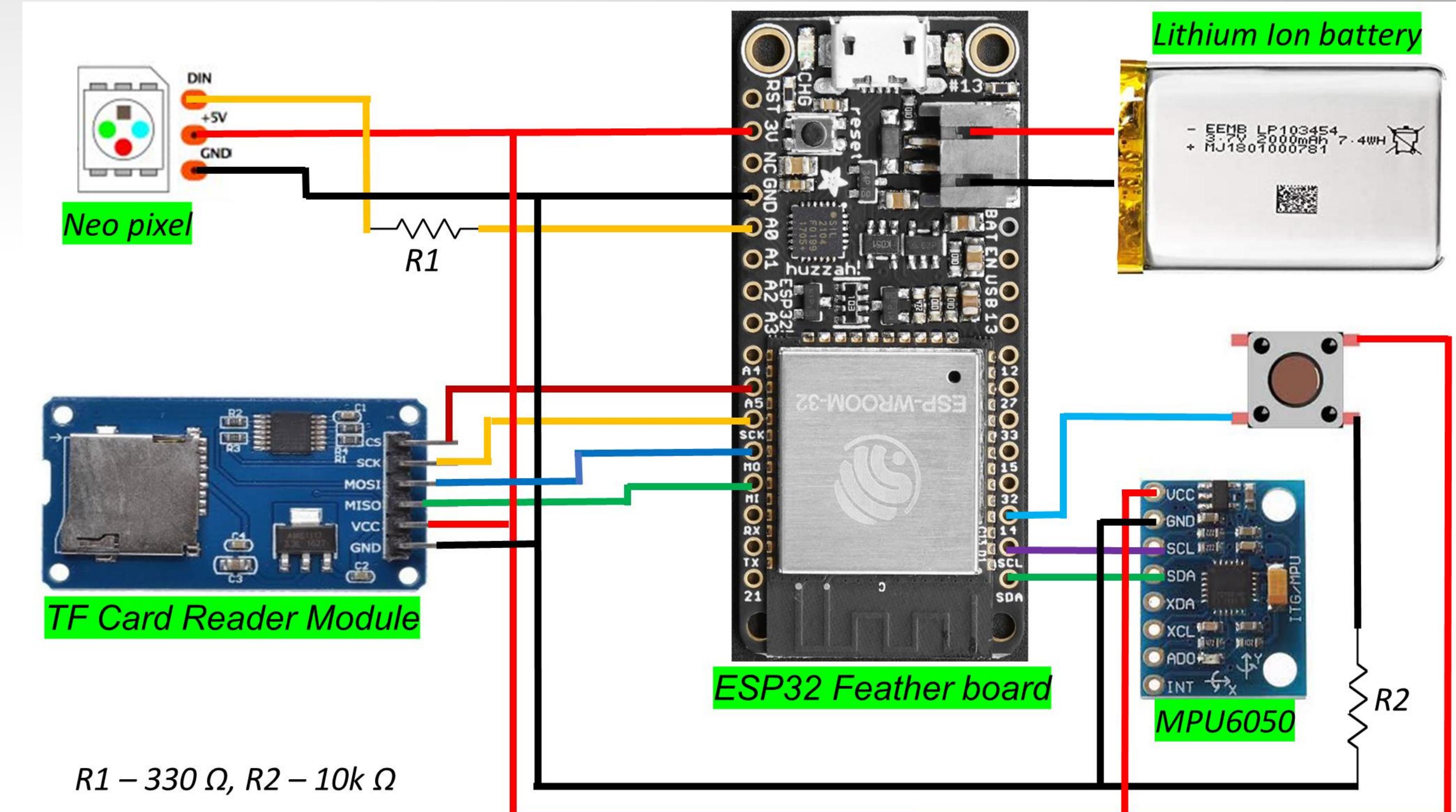
First Development

- But the gyroscope measurements along Z-axis are not similar
- Only accelerometer values are more suitable for developing real-time algorithm



Second Development

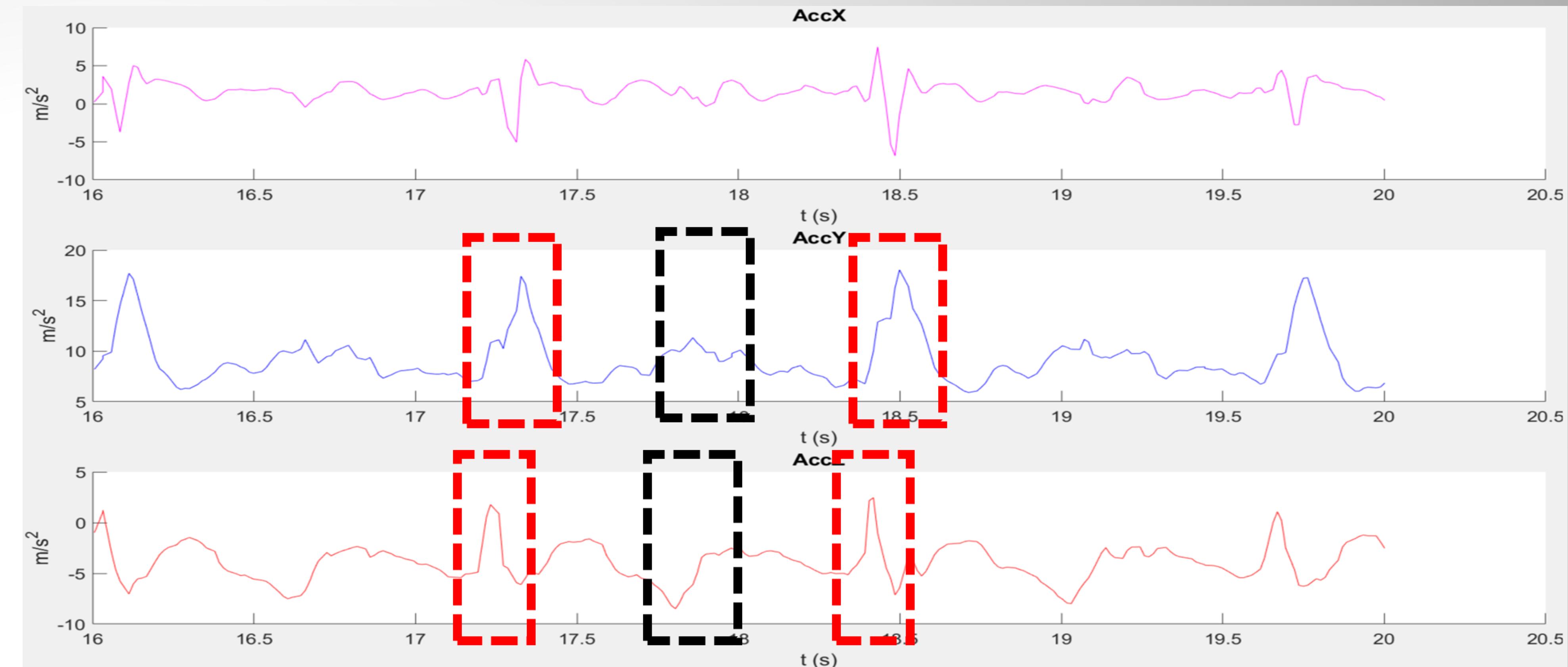
- Designed wearable device
 - MPU6050 sensor
 - ESP32 Feather board ⚡
 - LED - Neo pixel
 - Button
 - TF card reader module ⚡
 - Waist belt ⚡
- Waist belt
 - Soft fabric material
 - Adjustable bands



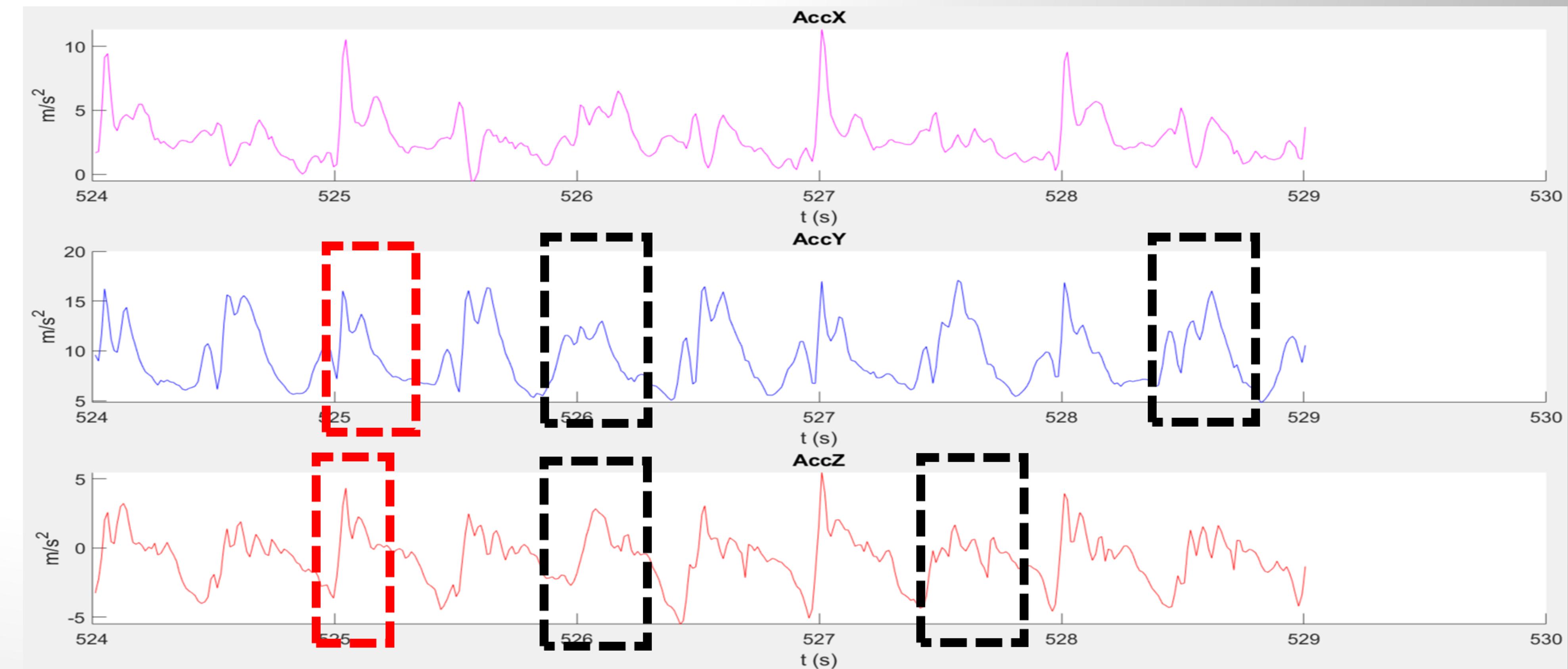
Second Development

- Observed walking patterns for users with prosthesis
- Peaks recorded during heel-strike event looked similar to users without prosthesis (red dotted box)
- There are heel-strike events where identification of peaks are difficult (black dotted box)
- There are more inconsistencies in the patterns

User with prosthesis on right knee

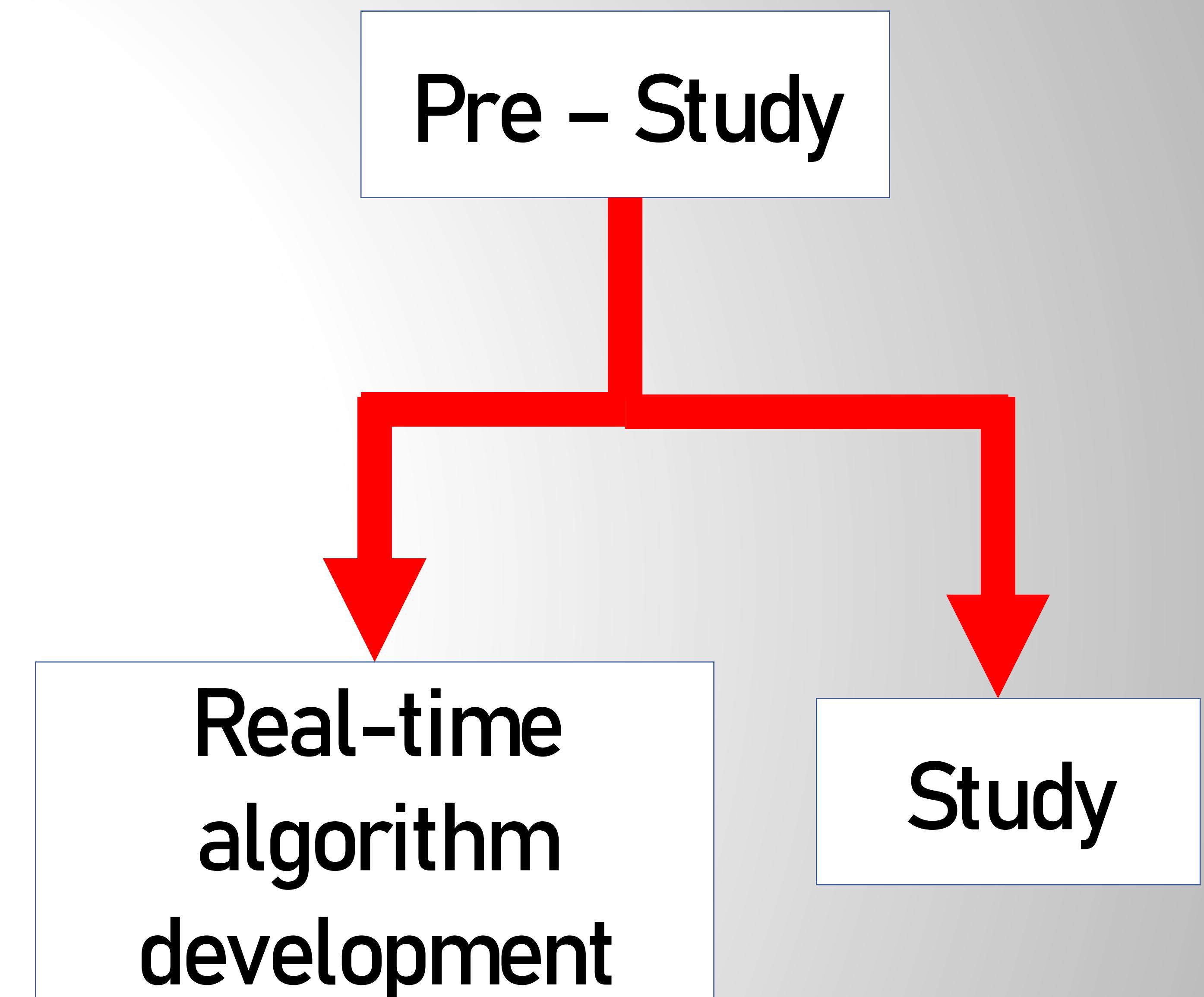


User with prosthesis on left hip

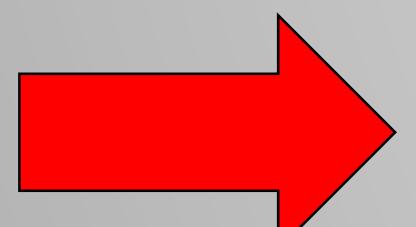


Pre-Study Conclusion

- More users walking patterns are required to analyse the criteria for asymmetry for walking
 - With prosthesis
 - Without prosthesis
- Verification of the hypothesis
- Need for pressure sensor
 - To confirm/understand the heel-strike events
- Validation of the real-time algorithm

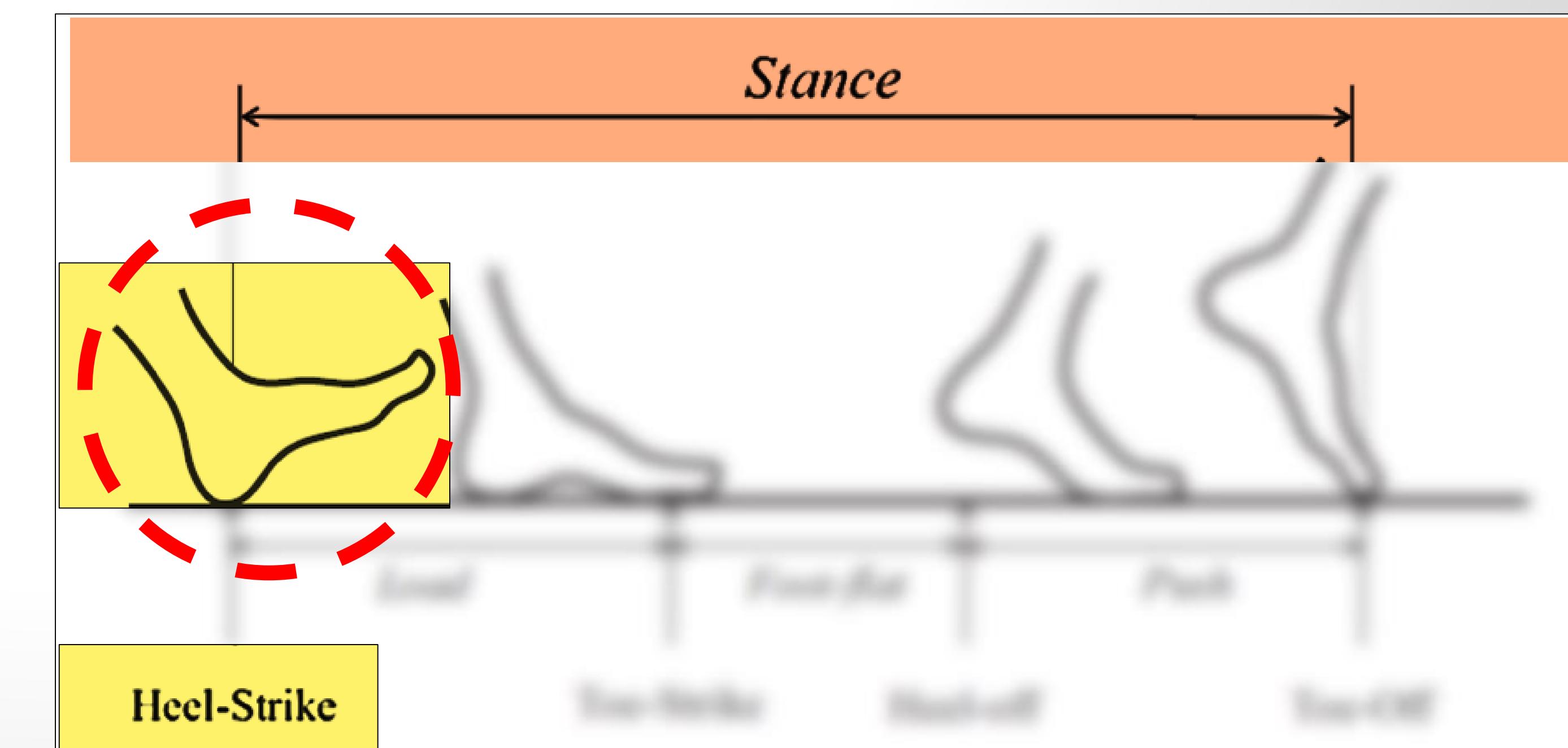


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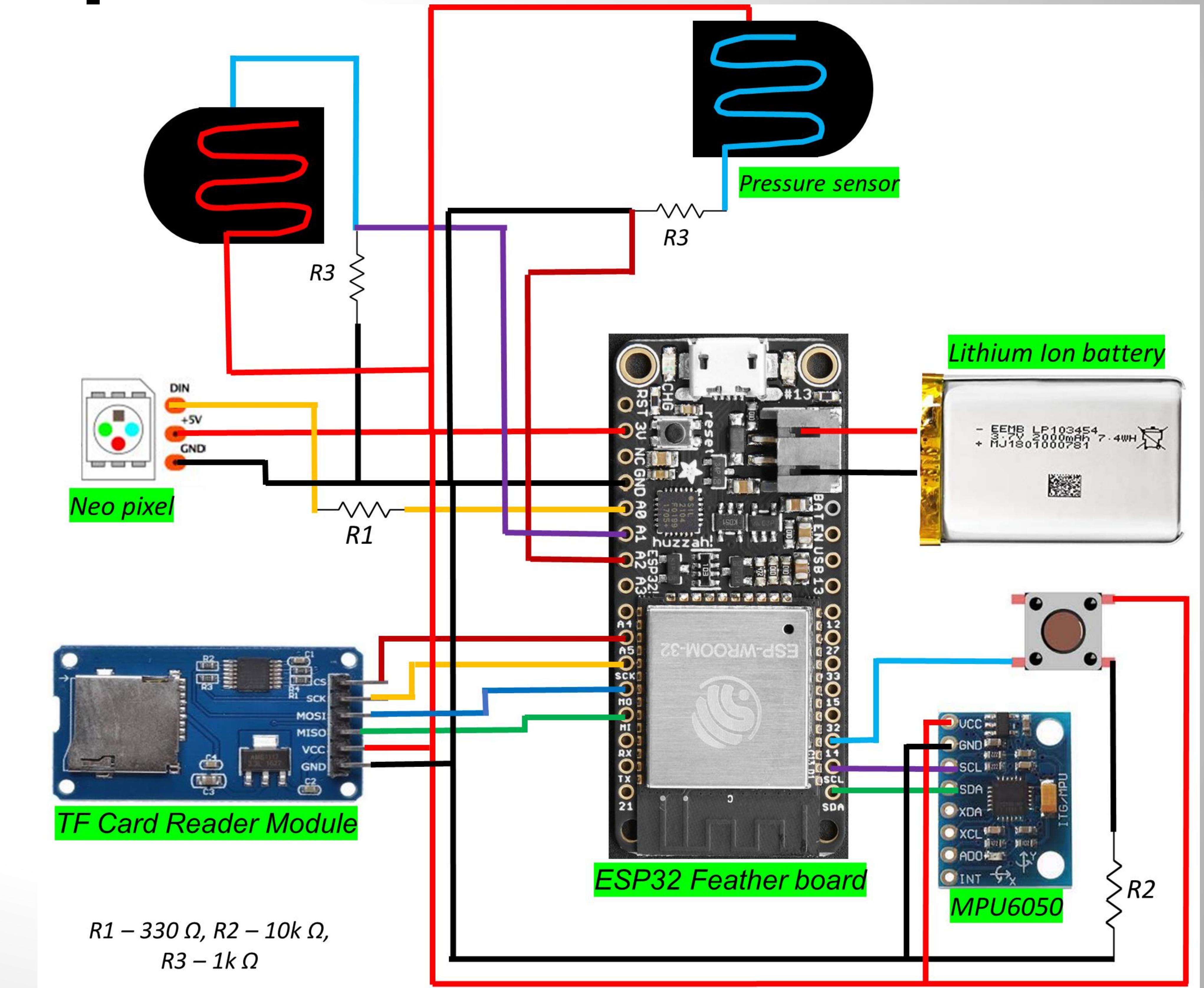
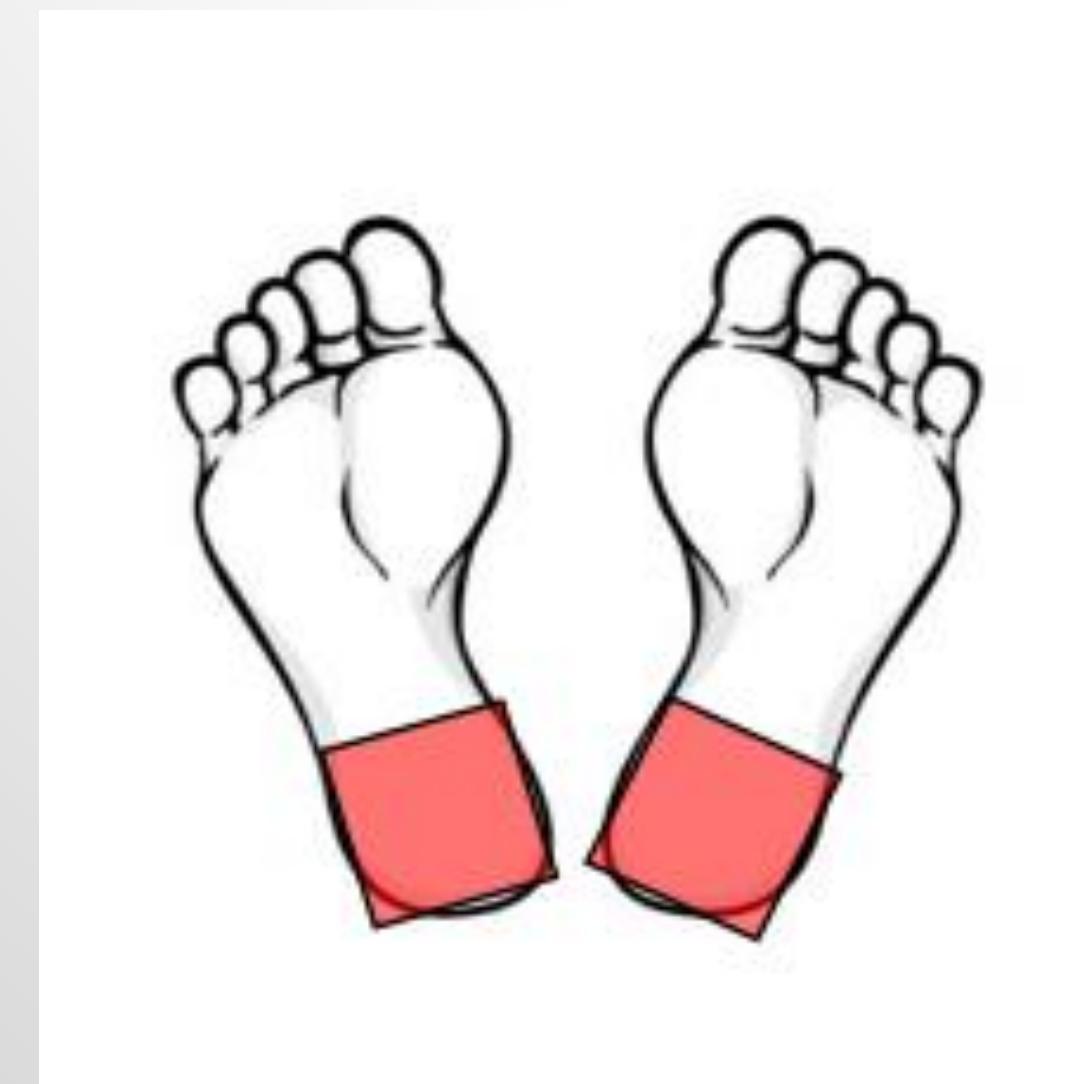
Study

- Temporary addition of pressure sensors
- Study procedure
 - Participants with prosthesis
 - In collaboration with the head physiotherapist Ulf Kaupschfer
 - Personal Communication Physiotherapeut at Ambulantes Physiocenter Gronau, Germany,
 - Users with hip prosthesis
 - Users with knee prosthesis
 - Participants without prosthesis
 - Heel-strike event



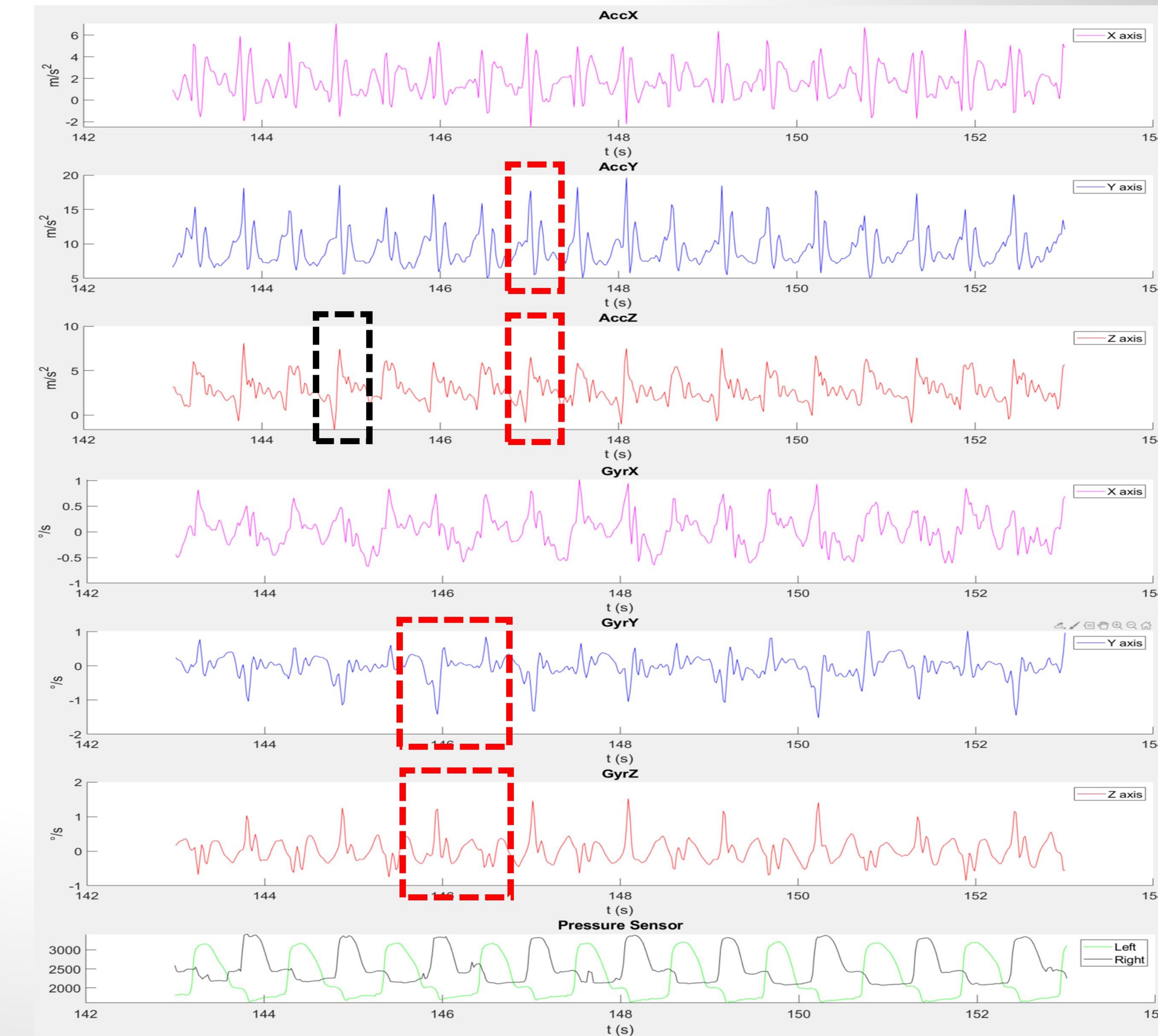
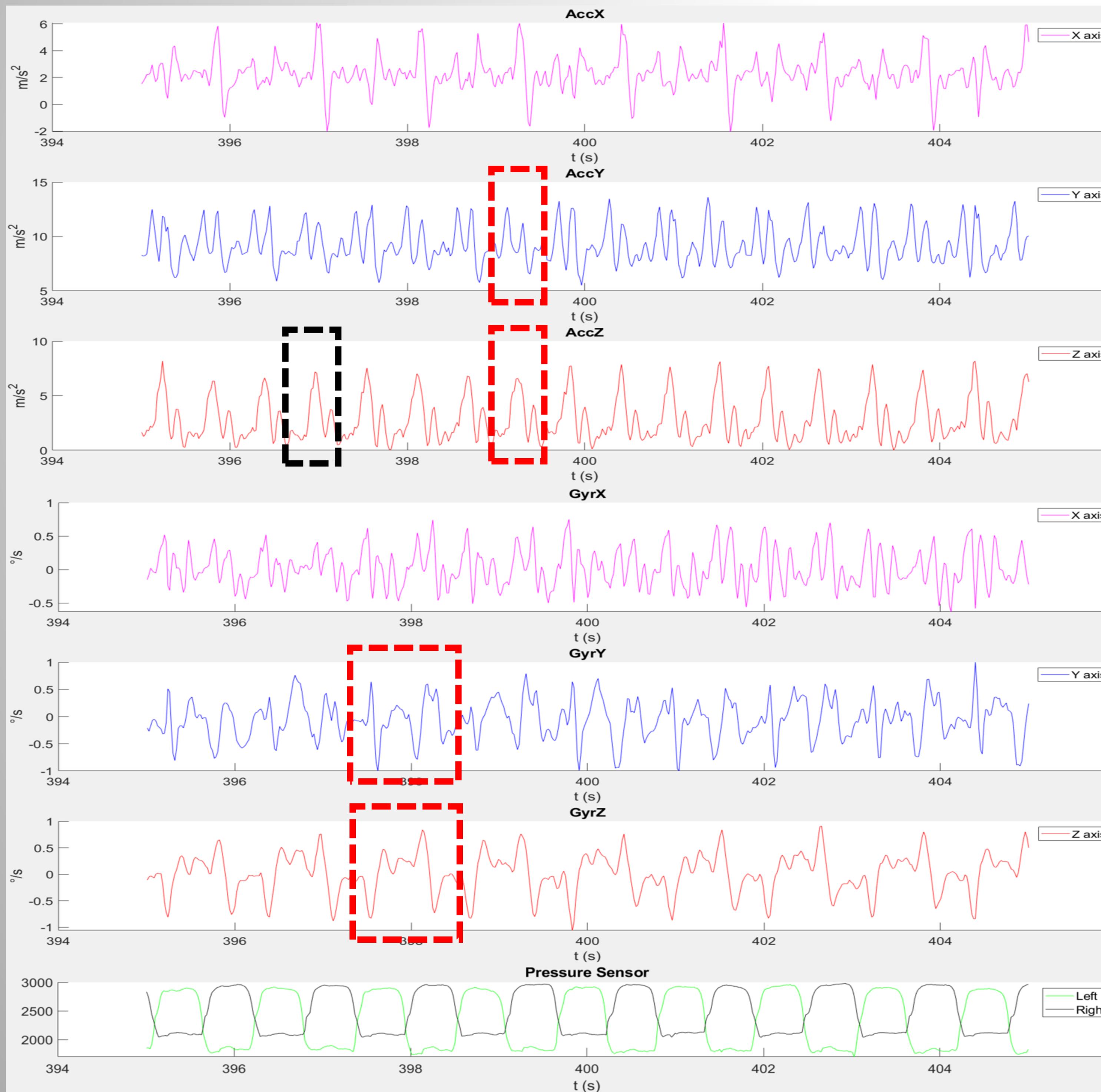
Temporary addition of pressure sensors

- Designed wearable device
 - MPU6050 sensor
 - ESP32 Feather board
 - LED - Neo pixel
 - Button
 - TF card reader module
 - Waist belt
 - Pressure sensors ⚡



Study Results – Users Without Prostheses

- Acceleration along Z-axis is consistent
- Repeating patterns along Y-axis and Z-axis

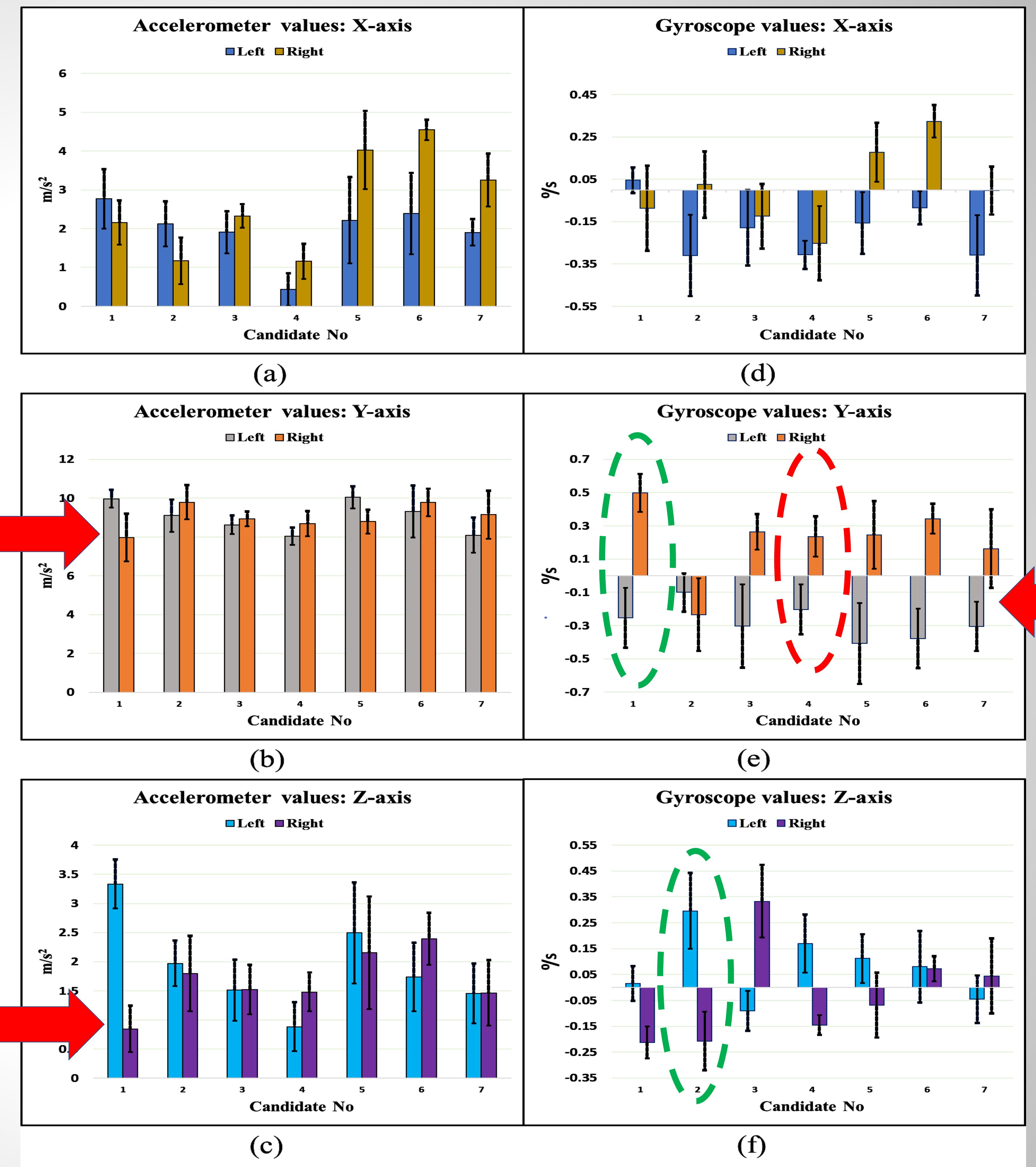


Study Results –

Users

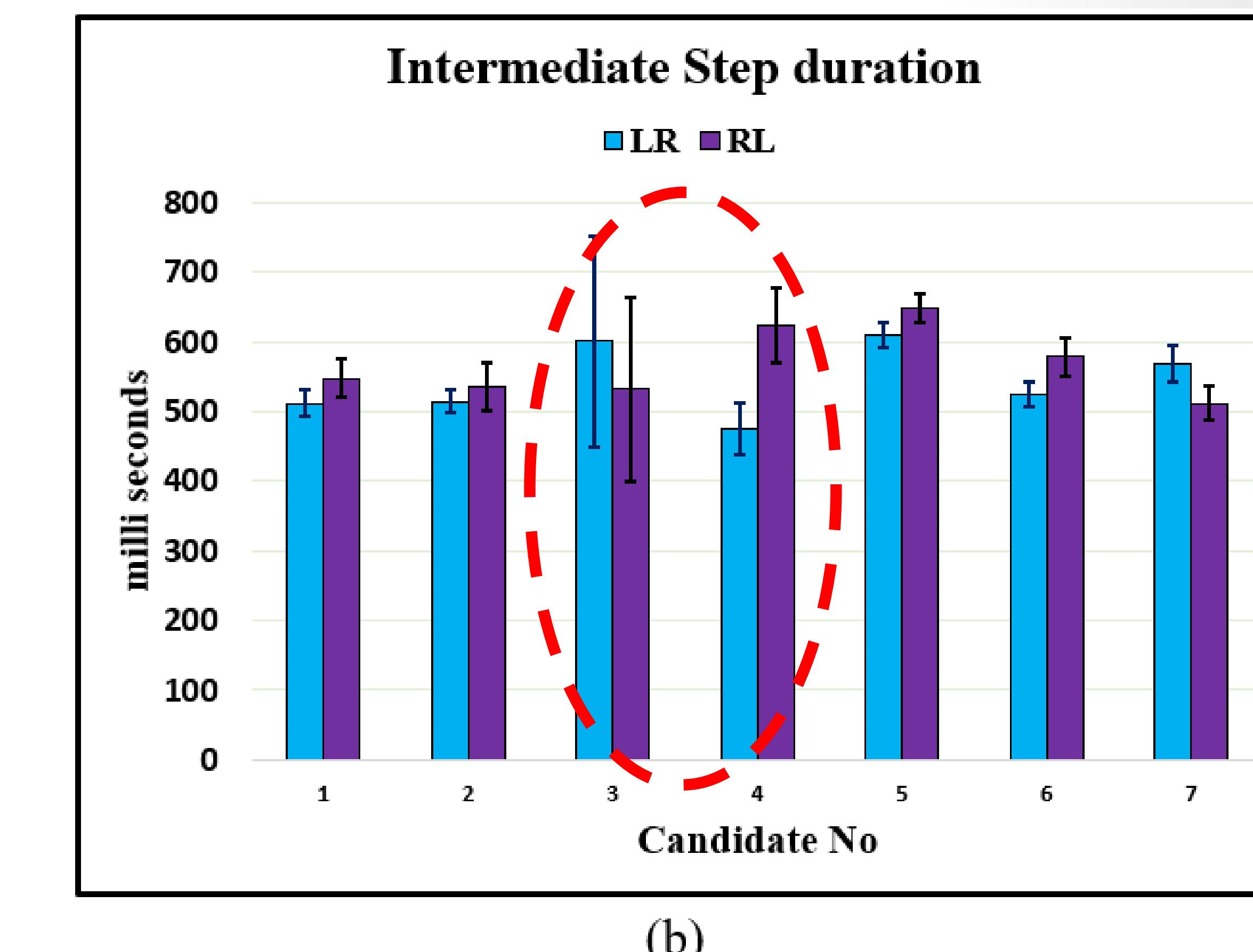
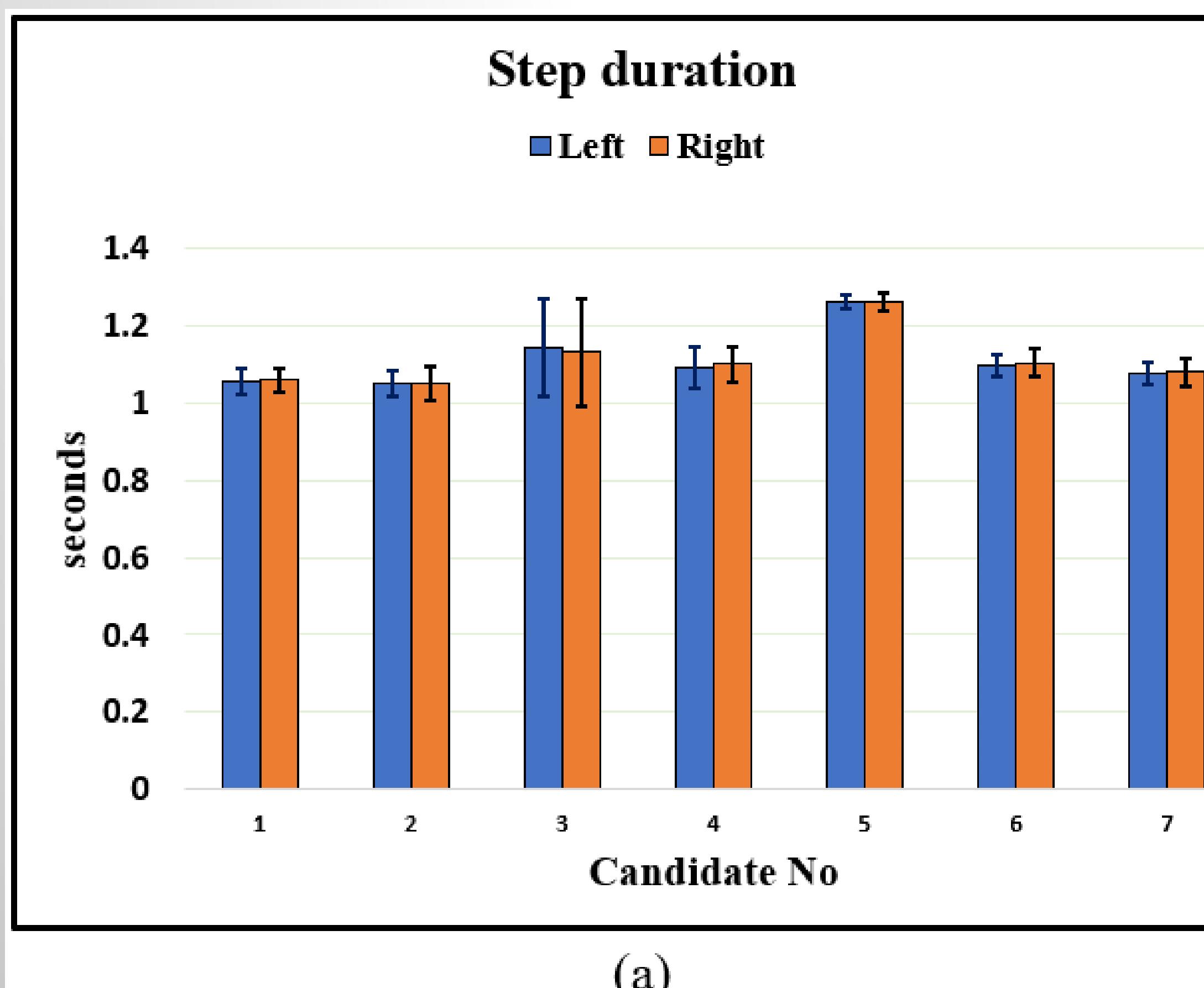
Without Prosthesis

- Linear accelerations and angular velocities of one foot are higher than the other foot
- Angular rotation measurements along Y-axis and Z-axis are opposite
- Angular velocities are opposite in direction for each foot



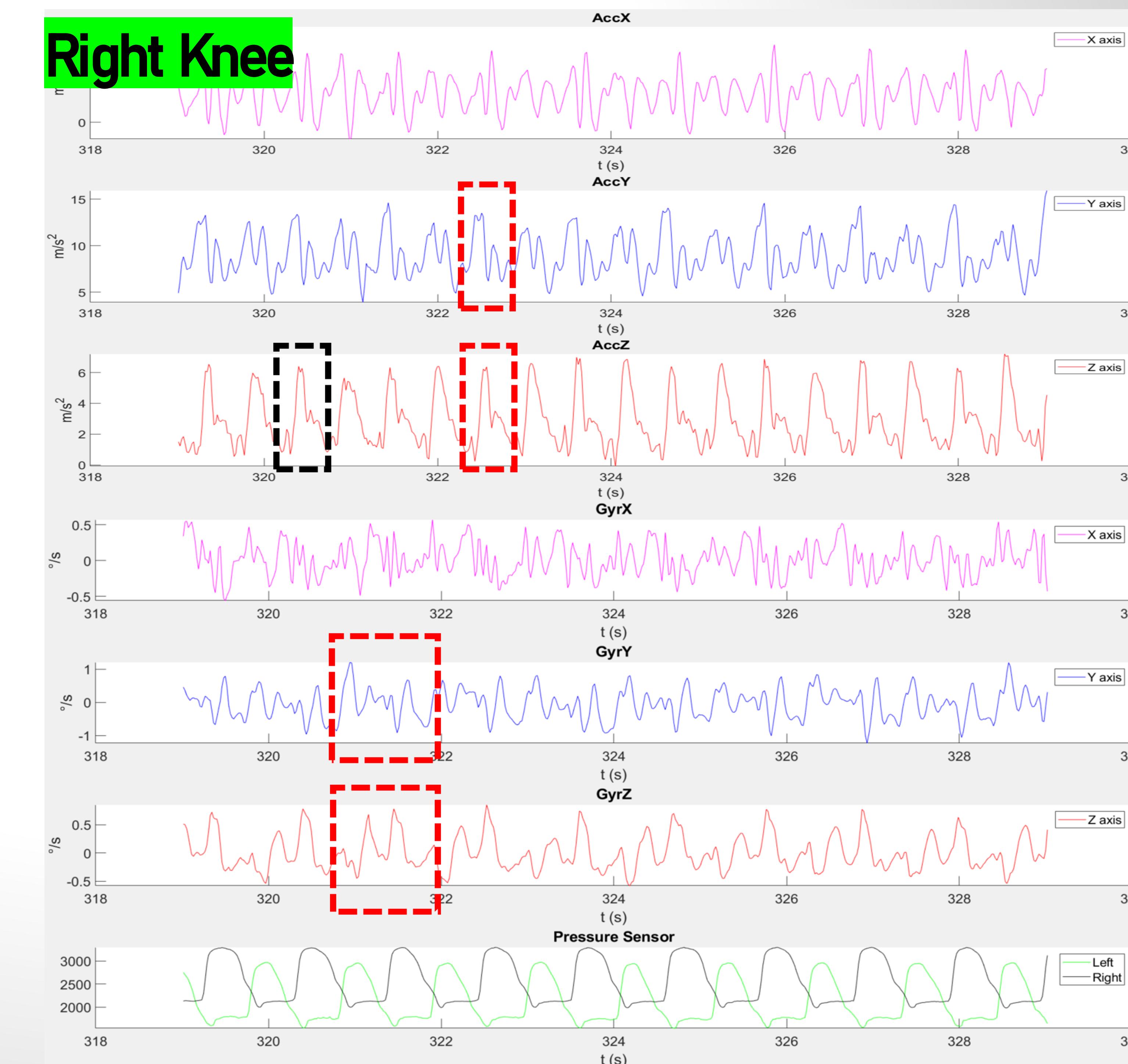
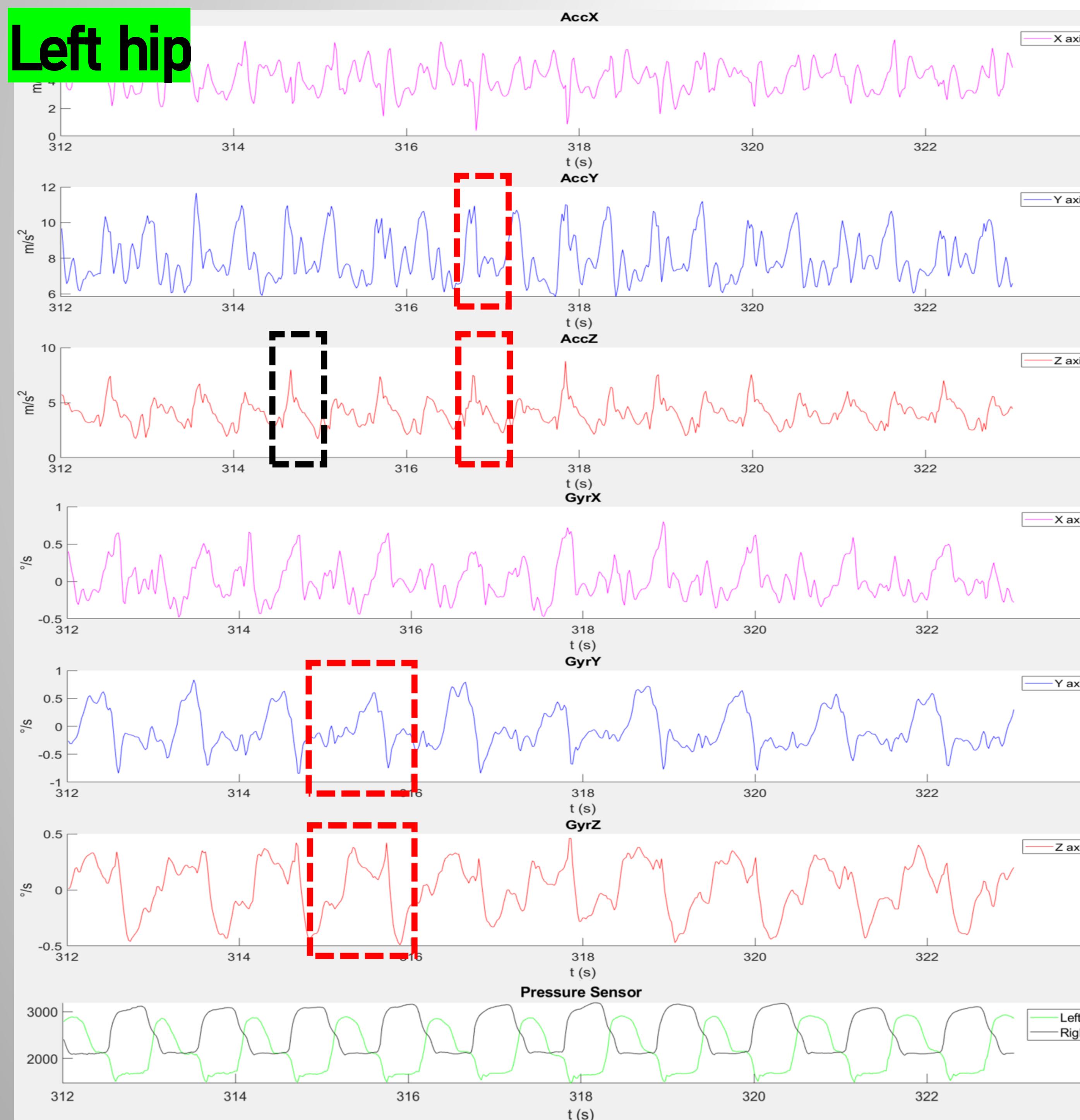
Study Results – Users Without Prostheses

- Step Duration
 - 1 sec to 1.2 sec
- Intermediate step duration
 - Left and right foot (LR) – 500 ms to 600 ms
 - Right and left (RL) – 500 ms to 600 ms



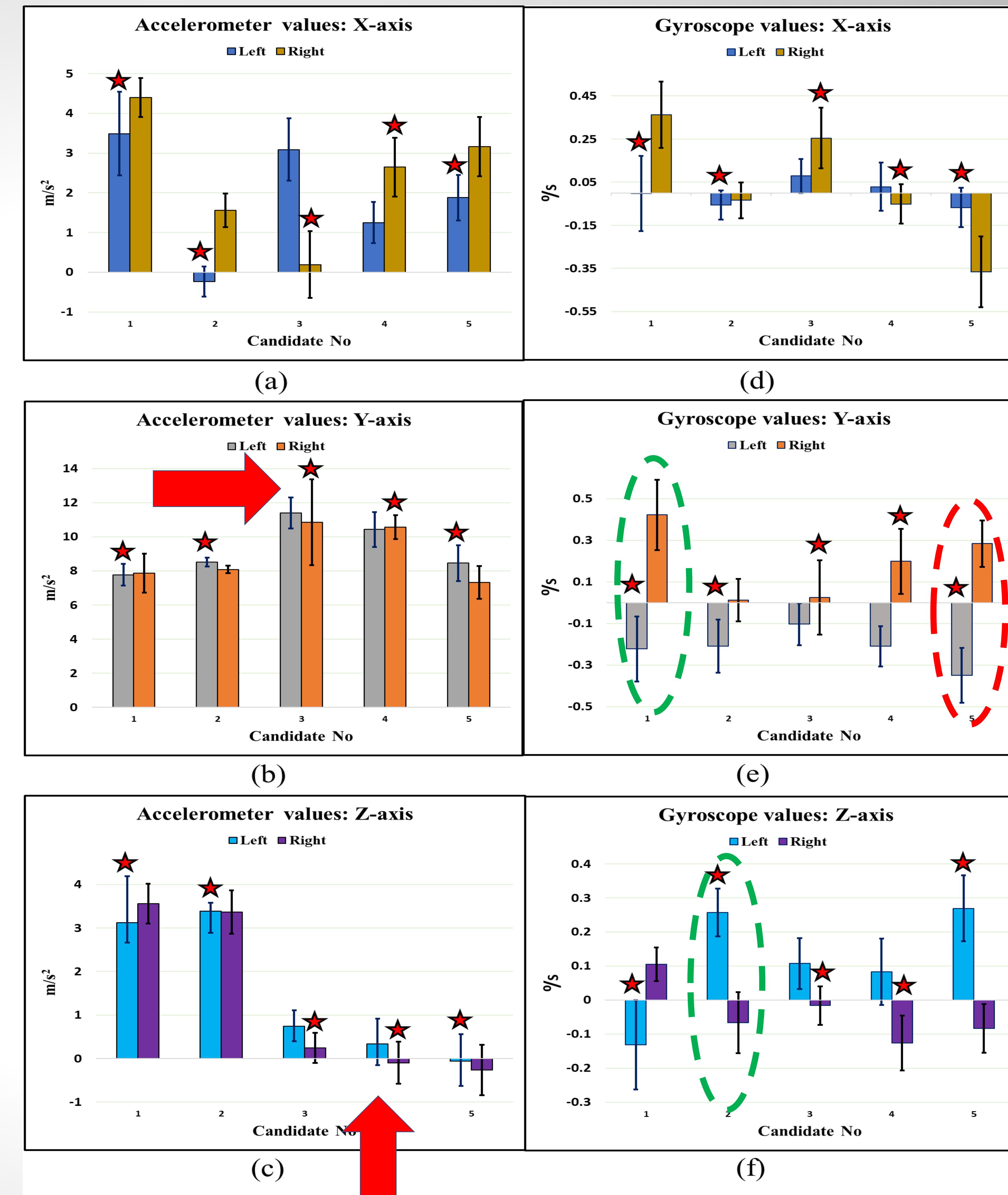
Study Results – Users With Prostheses

- Acceleration along Z-axis is consistent
- Repeating patterns along Y-axis and Z-axis



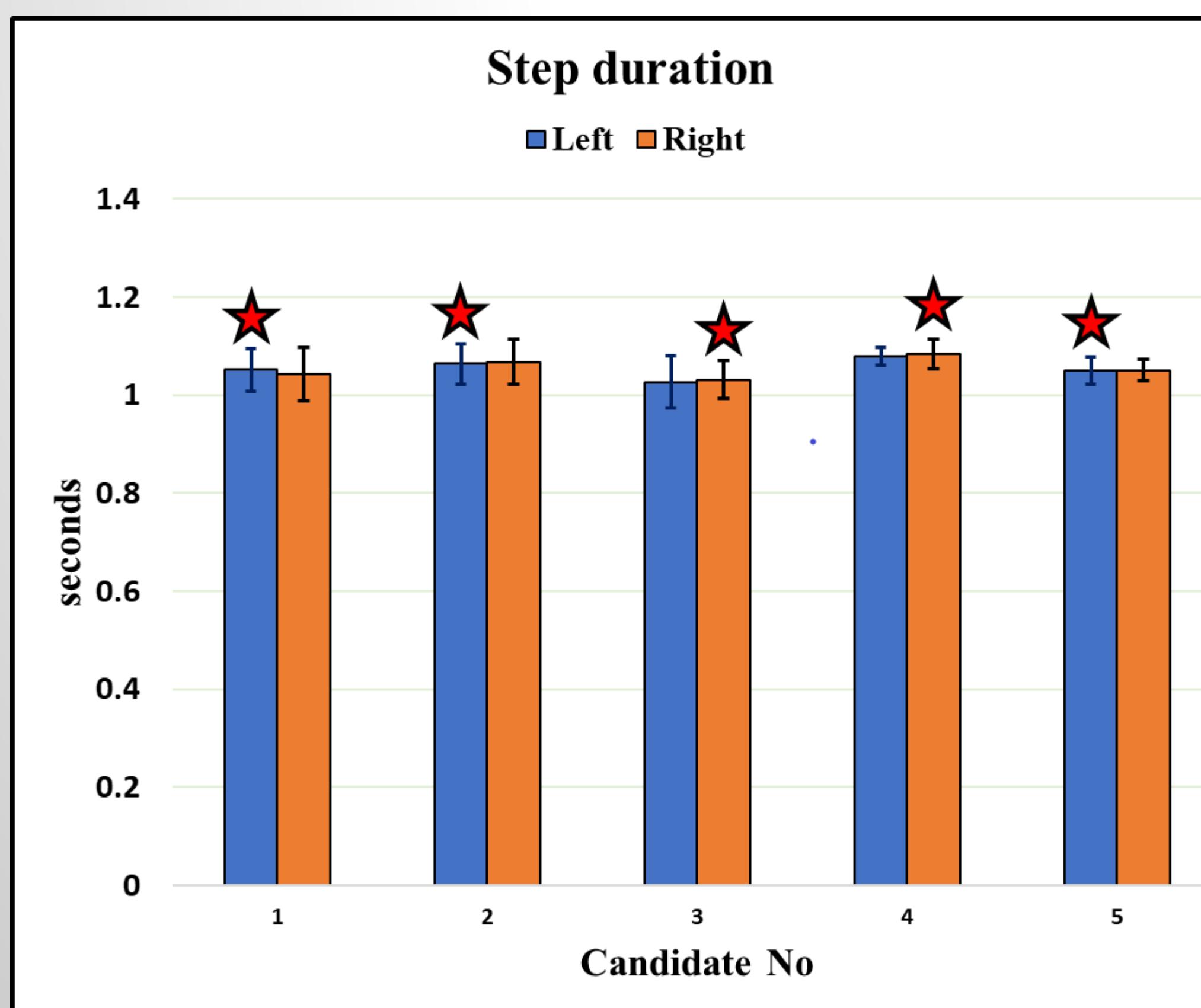
Study Results – Users With Hip Prosthesis

- Linear accelerations of few candidates are small in Z-axis but higher in Y-axis
- Angular rotation measurements along Y-axis and Z-axis are opposite
- Angular velocities are opposite in direction for each foot

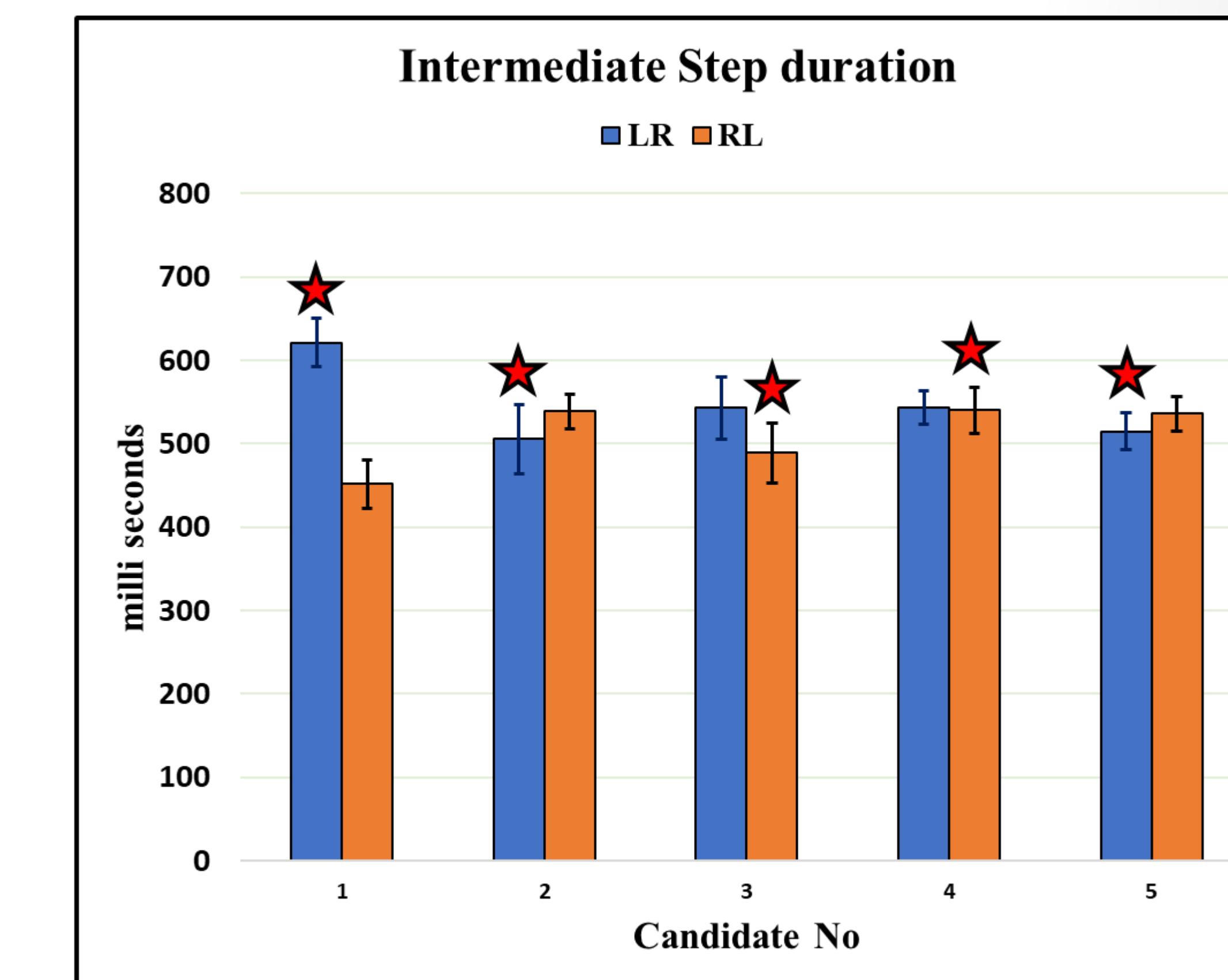


Study Results – Users With Hip Prostheses

- Step Duration
 - ≈ 1 sec
- Intermediate step duration
 - Left and right foot (LR) – 500 ms to 550 ms
 - Right and left (RL) – 500 ms to 550 ms



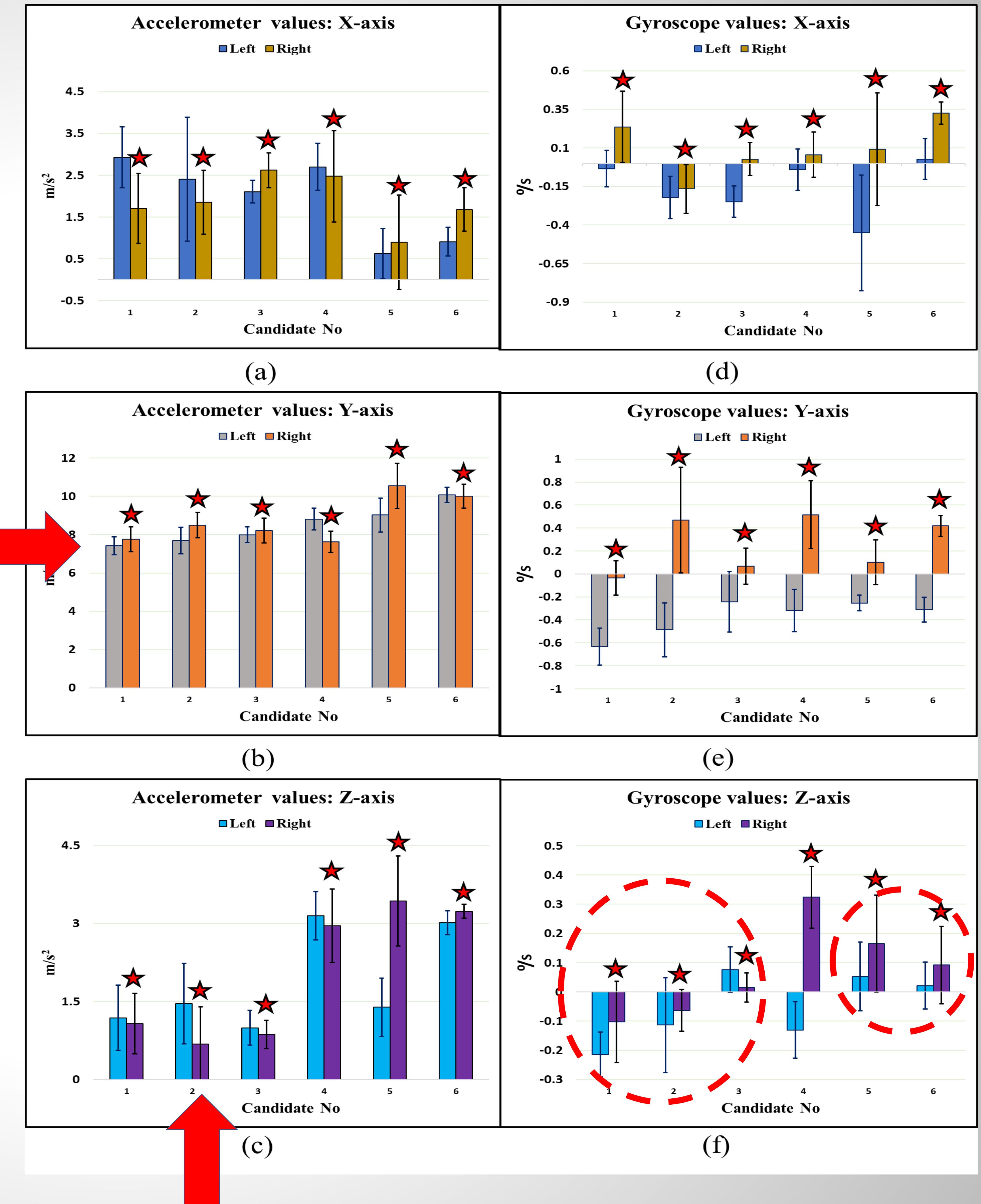
(a)



(b)

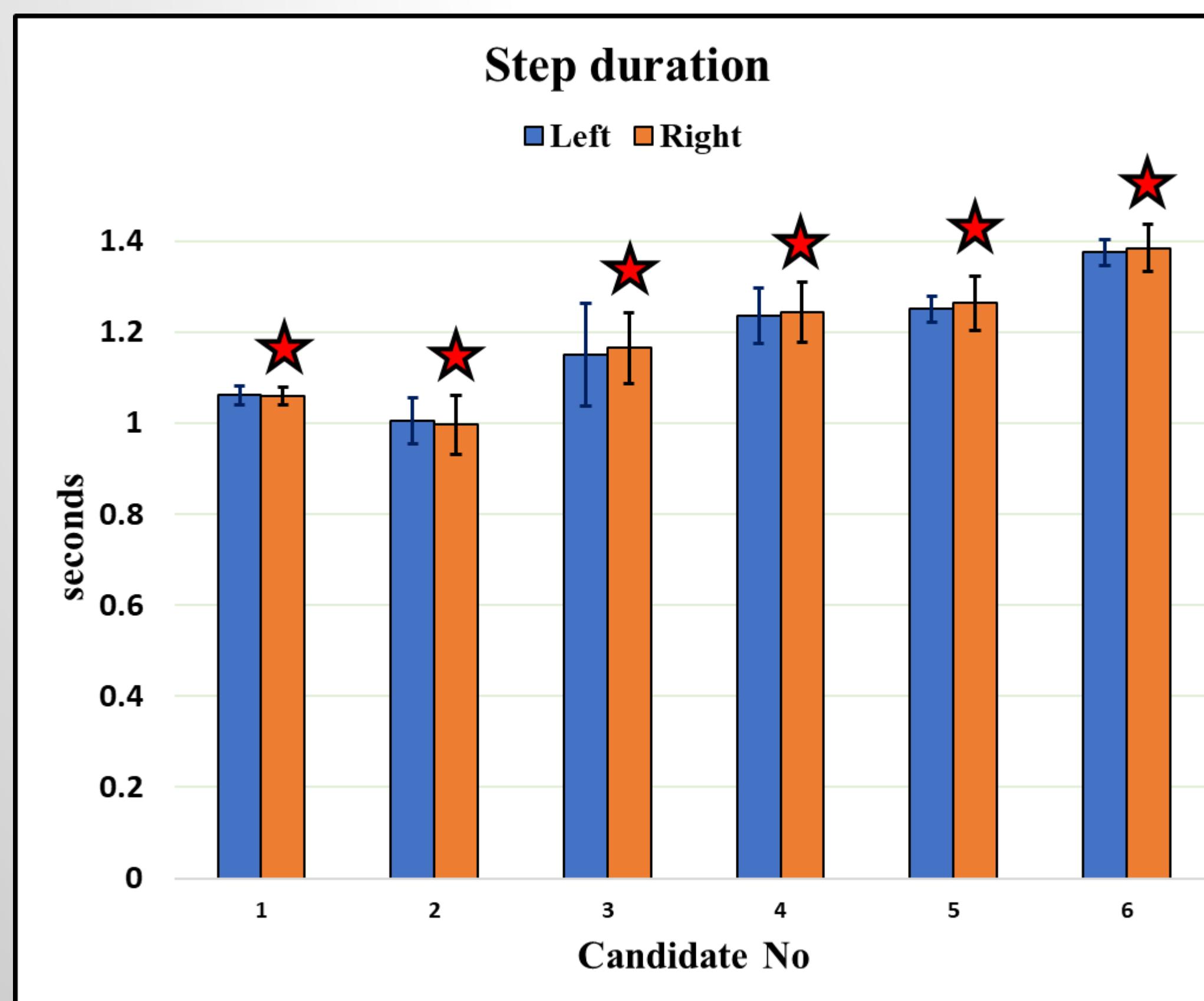
Study Results – Users With Knee Prosthesis

- Linear accelerations of few candidates are small in Z-axis
- Angular rotation measurements along Y-axis and Z-axis are opposite
- Angular velocities are  in the same direction for each foot (Z-axis)

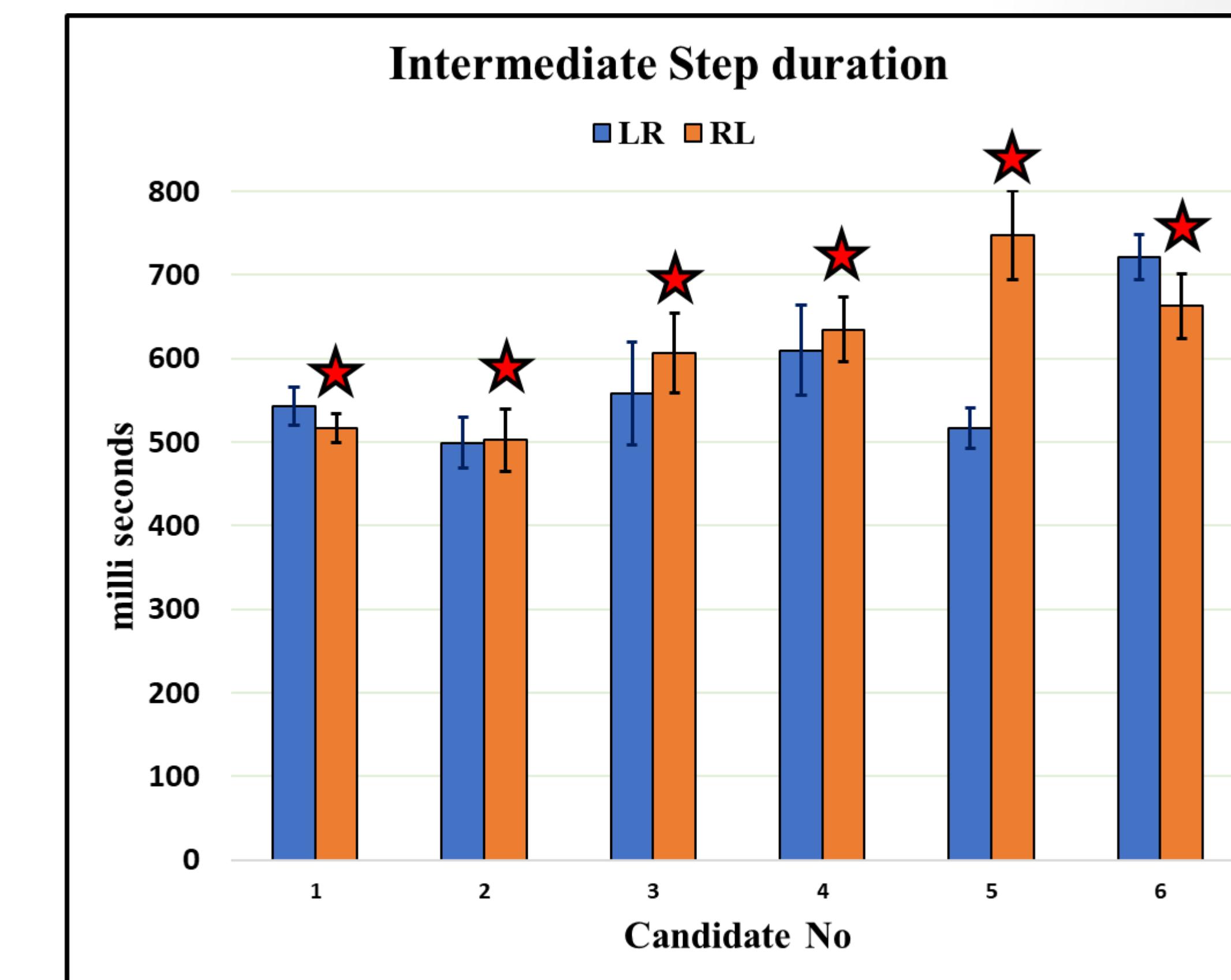


Study Results – Users With Knee Prostheses

- Step Duration
 - 1 sec to 1.3 sec
- Intermediate step duration
 - Left and right foot (LR) – 500 ms to 650 ms
 - Right and left (RL) – 500 ms to 650 ms

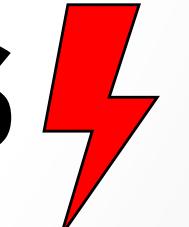


(a)



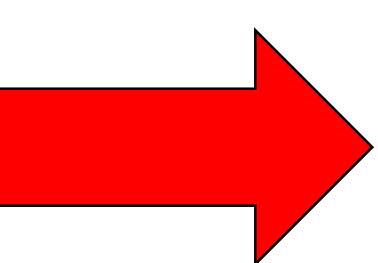
(b)

Study Conclusion

- Walking patterns recorded for users with and without prostheses are different
- Linear accelerations recorded similar values
 - Slightly less values along Y-axis for participants with prosthesis
- Angular velocities presented more differences
 - Users pelvis rotation is in one direction for both feet heel-strikes
- Intermediate step duration recorded similar results 
 - This observation negates the hypothesis
 - No considerable difference to distinguish the user with or without prosthesis
 - Real-time algorithm no longer capable to distinguish the type of walking 

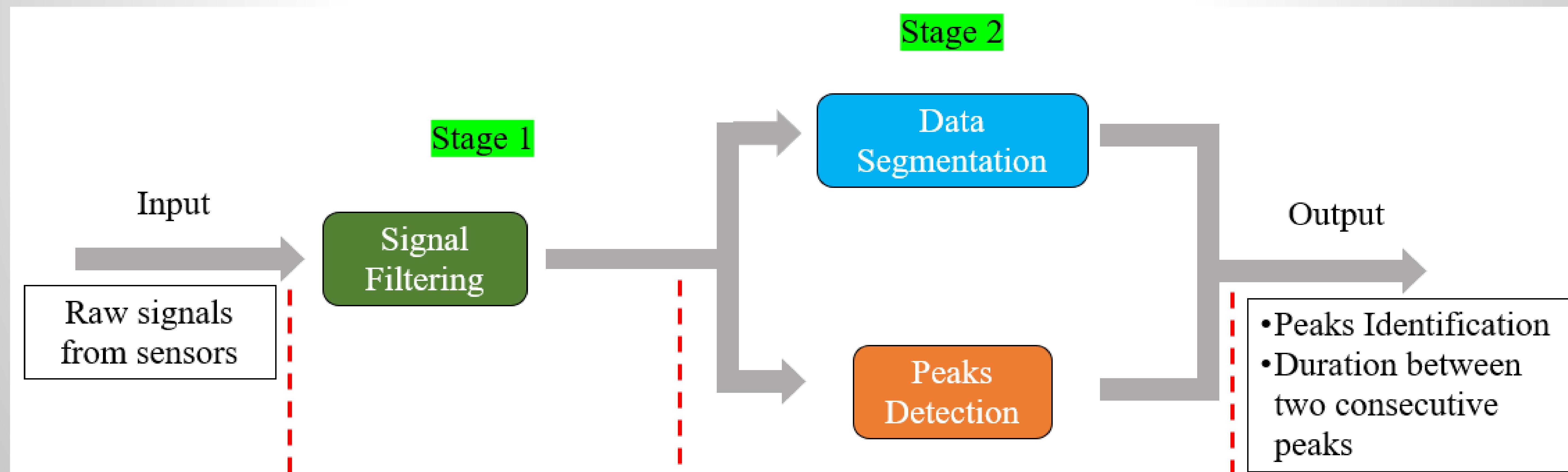
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Straight Forward Data Analysis Method

- Goal: To determine intermediate step duration
- Focuses only on the heel-strike event
 - Easy to verify the event in real-time
- Developed mainly using accelerometer values

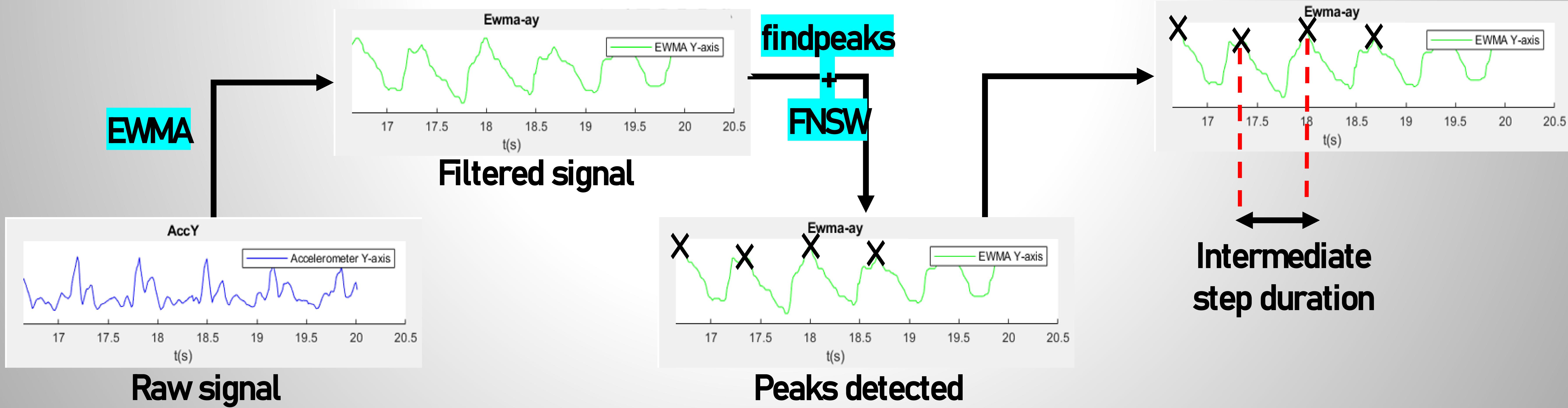


Straight Forward Data Analysis Method

- Signal filtering
 - Kalman filter
 - Exponential Weighted Moving Average (EWMA) 

- Peaks detection
 - Z-score Peak detection
 - `findpeaks` function from MATLAB 

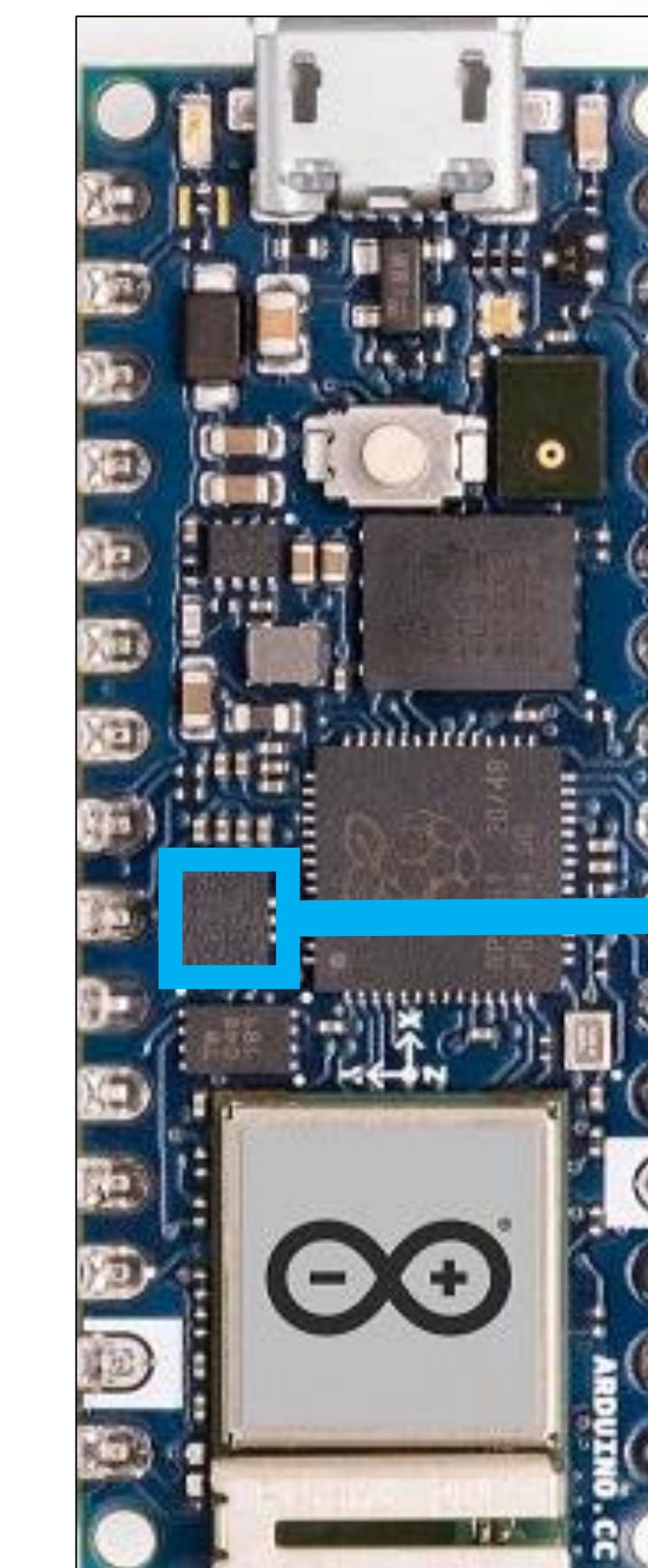
- Data segmentation
 - Static Fixed-size Non-overlapping Sliding Window (FNSW)



Machine Learning

- Machine learning
 - Capable of focussing on every event in the walking activity
 - Window sizes (number of samples/ duration)
 - It extracts a feature using accelerometer and gyroscope values
 - Uses this feature classification is done i.e. user walking is symmetric or asymmetric
- Device
 - Arduino Nano Connect
 - On board IMU sensor
 - Dedicated machine learning core capable of running decision tree algorithms

Arduino Nano RP2040 Connect



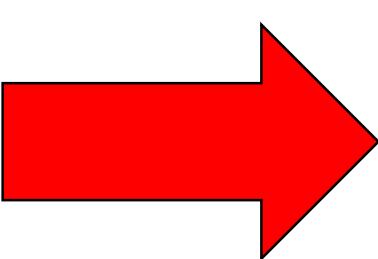
Procedure

- Data recorded from study
 - Symmetric
 - Asymmetric
- Segmentation
 - Window sizes
 - ≈ 3 sec, ≈ 2 sec, 1 sec
- Feature: Variance
- Classifier: REPTree
- Accuracy of detecting the user walking is symmetric or asymmetric
 - 96.96 % for window size of 3 sec i.e. almost equal to 3 steps taken by user

Window Size (in sample points)	154	102	52
Window Size (in seconds)	≈ 3	≈ 2	1
Classification Accuracy	96.9697 %	95.3177 %	93.2031 %
Kappa	0.9356	0.9014	0.8566
Mean Absolute Error	0.0474	0.0664	0.0929
Root Mean Squared Error	0.1716	0.2063	0.2426
Relative Absolute Error	9.9935 %	14.0024 %	19.5823 %
Root Relative Squared Error	35.2492 %	42.3746 %	49.8203 %
Size Of the Tree	9	9	39

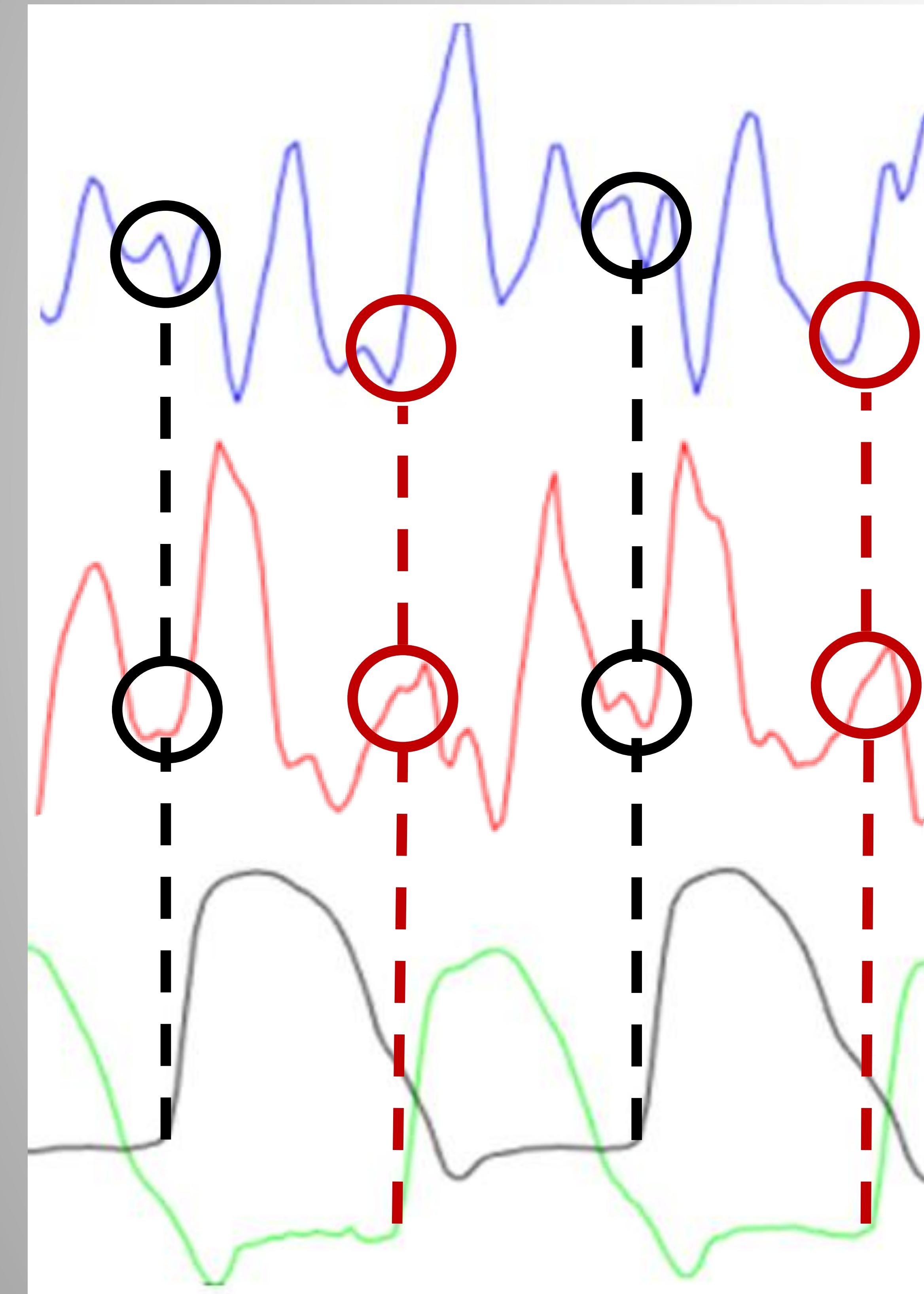
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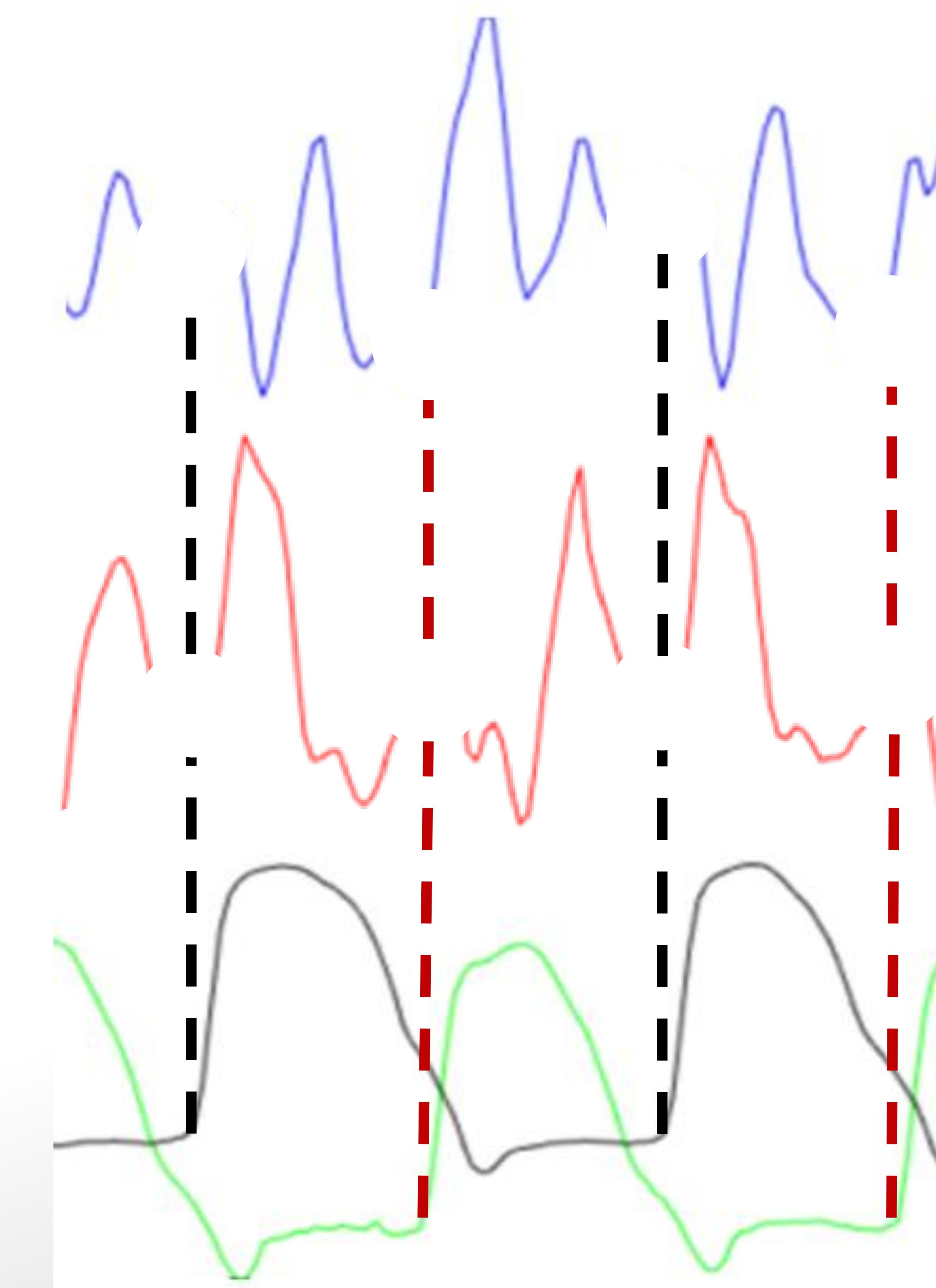


Gait Abnormalities In Hip/Knee Prostheses

Patients

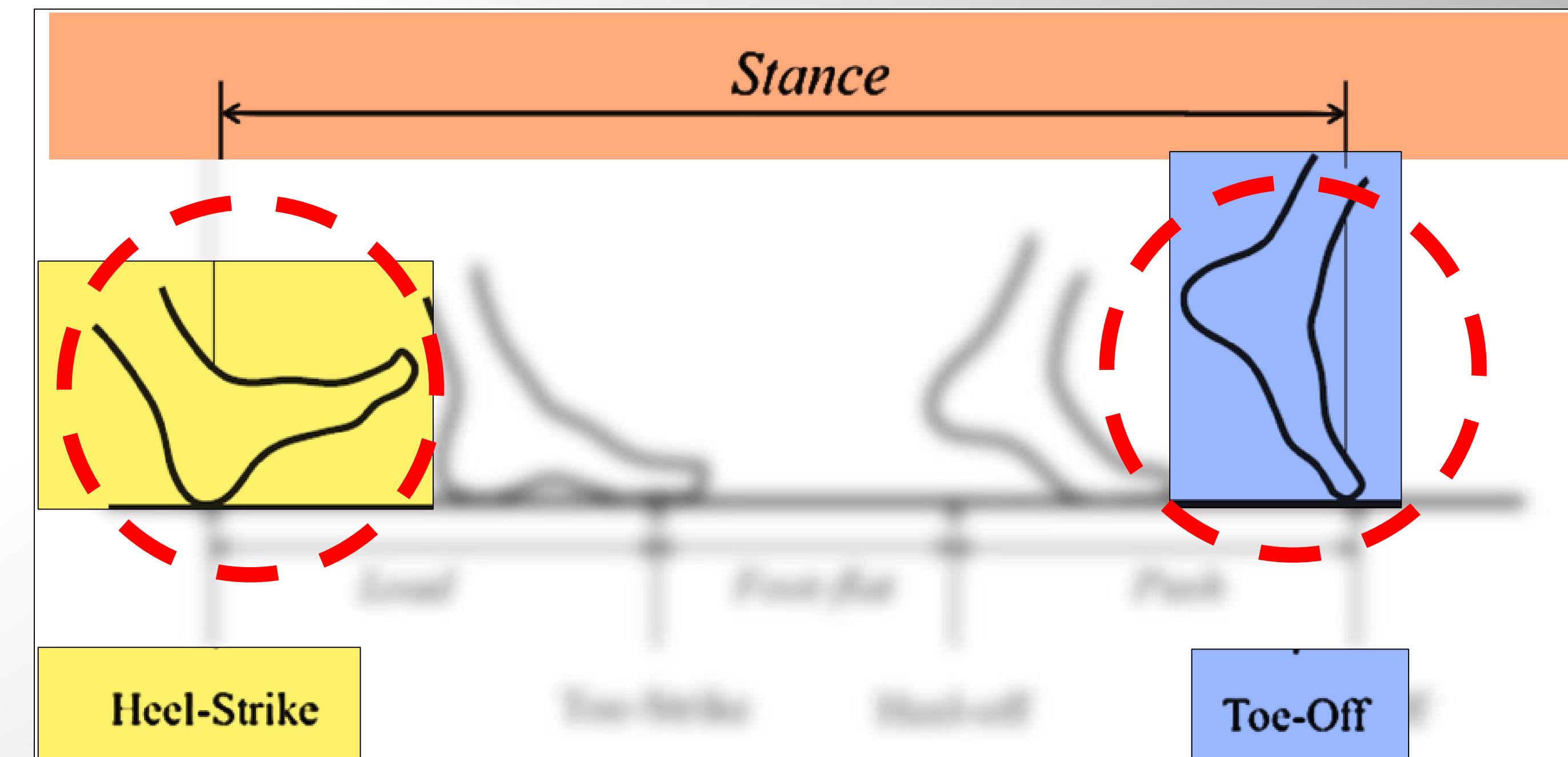
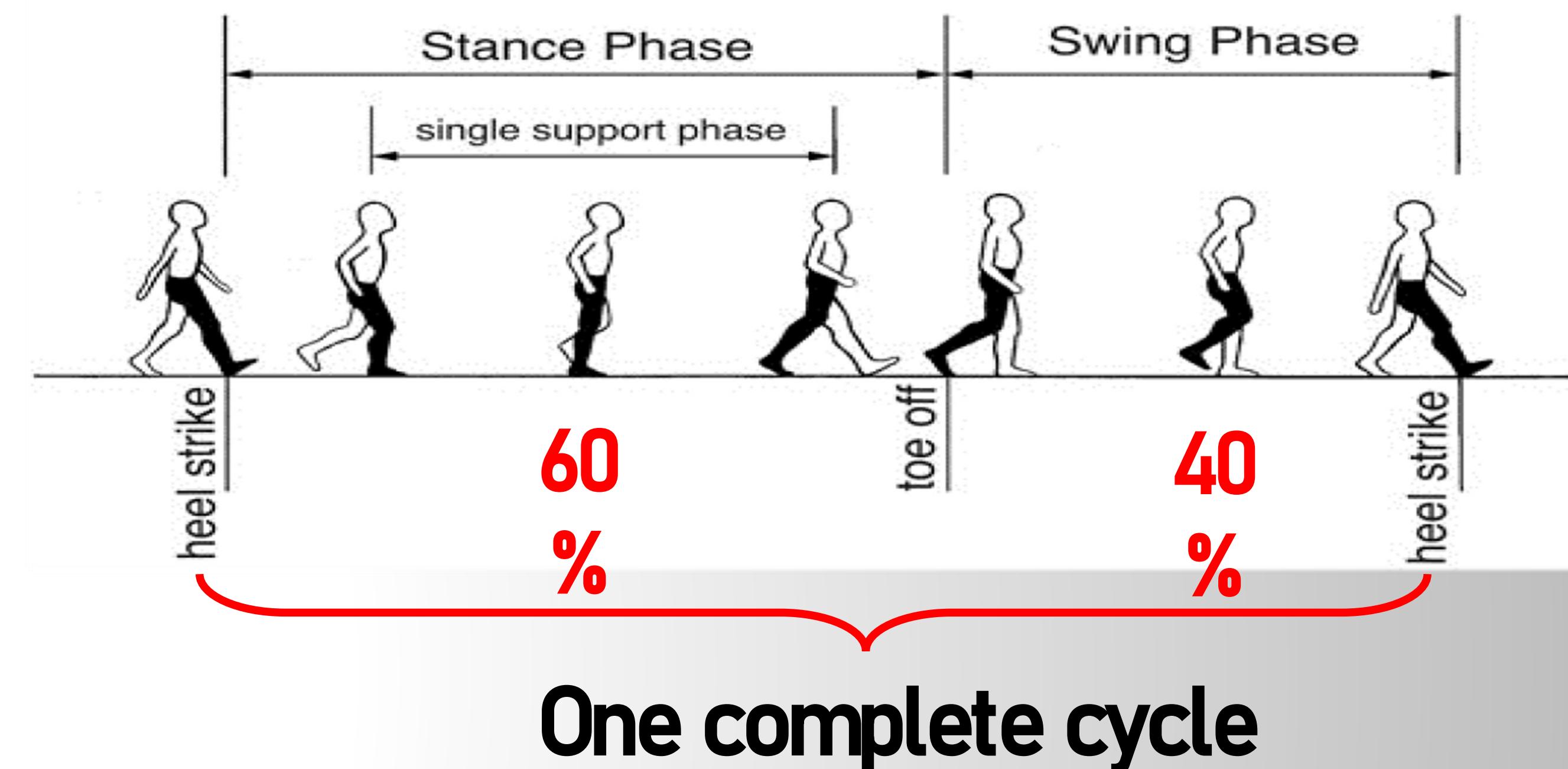


- Heel-strike event
- Remaining event in walking
- Difficulties:
 - One sensor capturing both legs movement
- Post processing the collected data
(future work)



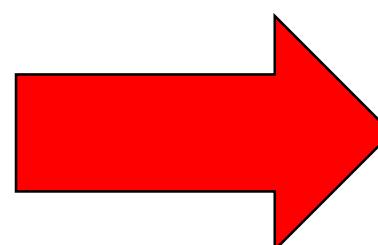
Identification Of Gait Patterns

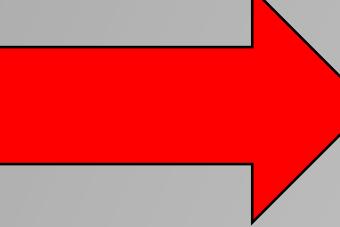
- Study
 - Heel-strike event is considered
 - Easy to identify and verify
 - To calculate intermediate step duration
 - Criteria for asymmetry in walking
 - Intermediate step duration
- Results from study
 - Negates the hypothesis – intermediate step duration is similar
 - Some visual observations during study
 - Knee bending is seen during swing phase
 - Additional pressure sensor in toe region
 - To identify toe-off event (future work)



Contents

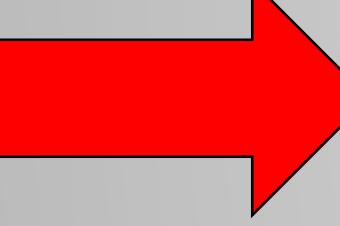
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[SQ1] What is the state of art in wearables for motor learning using haptic feedback?

- Sensors
 - Fixed setups – cameras/pressures mats
 - Post processing
- Wearable are used for data collection only
- No real-time feedback implementation



[SQ2] What gait abnormalities are characteristic for post hip/knee prosthesis patients?

- Observations
 - Diverse walking patterns
 - With and without prosthesis
 - Users with knee prosthesis
- Pelvis rotation is in same direction during both feet heel-strike events
- Step duration and intermediate step duration is similar
- Users with and without prosthesis

→ [SQ3] How to identify the relevant gait pattern?

- Straight forward data analysis method
 - Traditional approach
 - Hypothesis as criteria to identify the asymmetry in walking
- Machine learning method
 - Realization of hardware
 - Real-time
 - Matches wearability requirements
 - Binary classification
 - 96.96 % accuracy

→ [SQ4] What contributes to wearability for a haptic feedback system?

- Waist belt designed matches the wearability requirements
- Lower back location
 - Capable of identifying asymmetries



[SQ5] What is effective and simple haptic feedback for gait training?

- Cannot answer this question completely
 - Criterion for identifying the asymmetry for hip/knee prosthesis is pending
- Haptics for good starting point
 - Implemented for sports
 - Running
 - Rock climbing
- More experimentation is required

[RQ] How to design a wearable that give haptic feedback for motor learning of patients who undergo hip/knee prostheses

- Identification of asymmetries in walking
 - Study
 - The parameters measured during heel-strike could not provide a strong criteria to identify symmetry
 - It also showcased the intermediate step duration is also similar
 - Straight forward data analysis method
 - Focused around heel-strike event only
 - Developed based on hypothesis
 - Machine learning
 - Showcased that identification of walking of user -symmetric or asymmetric- is possible
 - Need to consider all the events in walking
- Feedback
 - This is the later part of designing a wearable device
 - Future work

Questions?

Questions?

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