**Predictive Processing and temporal predictability in visual domain**.

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**Introduction :**

Predictive processing is framework which explains how does the brain interacts with the external environment through sensory modalities. The core idea behind all the predictive processing theories is that the brain predicts about the environment around it and develops a generative model. The model is constantly updated through the comparison of predicted and actual stimuli. This process follows a cortical hierarchy (processing hierarchy), the higher order brain areas makes a prediction (top – down descending activation) and the lower order brain areas (bottom up ascending activations) gets the actual stimuli input. The comparison between both the actual and predicted input is termed as prediction error and this error signal is used to update the internal model of environment around us [1].

This framework has also been termed by different names like predictive coding, hierarchal predictive coding etc but the key elements remain the same *“Prediction”* and *“Prediction errors”* [2], [3]. It is well supported in literature that predictive processing framework has been able to account for underlying cognitive processes both in humans as well as animals [4]. Predictive processing accounts for visual perception [5][6] and auditory perception [7], speech perception[8], language [9] and music [10]. The framework is also used in explaining the abnormal functioning in neural disorders like autism [11], psychosis [12] and several others.

In this hierarchical framework, the input stimuli to the lower order brain areas may have several features. A visual stimulus may have features like edges, orientations, color, shape and other properties, whereas the audio signal might have features like volume, amplitude, frequency, pitch etc. These features forms the basis of perception and are related to the identity of the stimuli often contain the “WHAT” information. But in real life situation the timing of the input stimuli also matters a lot. You may see a car coming toward you on the road, even after having all the “WHAT” information features, it is really important to know the “WHEN” information to avoid a collosion. The same example holds valid in auditory domain i.e how fast or slow you listen to the input shapes your perception. This WHEN information has gained less interest compared to the WHAT information. These WHAT and WHEN features interact with each other and shape the human perception so there is also a need to understand understand the interaction of WHAT and WHEN in human perception. There have been attempts by Faidella et al [13] to understand this interaction in auditory domain, but the limitation of the EEG modality (restricted to source level inferences only)and experimental design did not shed proper light on this interaction. There were also attempts by Auksztulewicz et al [14] to study this interaction using ECOG data, but the less no of participants used and exclusion of an important factor i.e Attention, failed to investigate the proper interaction of this What and When.

Attention and Prediction both are top down processes, both affect human perception. Theories on prediction relate to neural (mental) models inferring about (present or future) sensory or action-related information, whereas theories of attention are about the control of information flow underlying perception and action. Both concepts are related and not always clearly distinguishable. [15] Whereas there have been a lot of evidence about the feature specific attentional abilities which means the focussed and divided attention can be dissociated [16][17][18]. This gives us motivation to investigate attention and prediction by designing an orthogonal task, where attention is diverted to one feature of the stimuli whereas the prediction is related to another feature. This design should analyse the prediction effects in less/diverted focus of attention.

Returning back to the WHEN information, this information about the stimuli might be either predictable or unpredictable (temporal predictability in general). Most of the experiments in predictive processing research have studied prediction effects with just two components i.e a cue and a target. This has been reported as match and mismatch prediction effects based on match/mismatch of cue and target. To investigate the effect of temporal predictability on prediction, there should be longer sequences of cue’s which will generate stronger predictions, helps to understand how does the temporable predictability affect the development of predictions.

In this experiment we focus on visual domain, interaction of WHAT and WHEN information and investigation the prediction effects in less focus of attention. We manipulated the attention of the participants to one of feature of the stimuli (cpd : cycles per degree of a gabor patch) and the prediction to the another feature (orientation of the gabor patch) in a series of previous stimuli in a sequence of four gabors. The feature having focussed attention is present at the Target. Here we plan to measure the effect of temporal predictability on the four gabor patches which are in less focus of attention.

The presentation of gabors may enhance the neural response or may also suppress the neural response based on temporal predictability. This kind of suppression or enhancement has been studies through different names like Neural adaptation, repeation suppression, repeatition enhancement, mnemonic filtering, decremental response and Neural priming [19]. On one side it is possible that temporal predictability could enhance repeatition suppression effect as there are two sources of information about the stimuli i.e timing and orientation. On the other side it is possible that the predictions are enhanced when the timing information is unpredictable as the system increase the reliance on the internal model to reduce the uncertainity of the external stimuli. We do so through conventional evoked analysis approach and advanced analysis like source reconstruction.

With the access to higher computational power and advanced machine learning methods, multivariate pattern analysis has gained a lot of interest in recent years. It is now possible to decode the orientation, position, identitity, angle, seen and unseen information from EEG and MEG signals at every millisecond or every sample [20][21], [22]. I will be interesting to decode the orientation of each presented gabors during less focus of attention, representing the developing predictions.

**Methods :**

**Participants :**

Seventeen (xx Females) took part in the present study with mean age xx, std- yy and age range xx- yy years. The ethical committee and scientific committee of Basque Center on Cognition, Brain and Language (BCBL) approved the experiment (following the principles of the Declaration of Helsinki) and each participant signed an informed consent form. Each participant was paid 10 € per hour for their valuable contribution. The participants were recruited from BCBL web participa and all the participants were free from any neurological and psychological disorders. All the participants had normal or corrected to normal vision.

**Experiment Design :**

To address the experimental questions, we developed an experimental paradigm in which participants were presented with simple visual stimuli (gabor patches) that could vary in a number of dimensions. Four gabor patches were presented for 200 milliseconds sequentially (with the inter-stimulus interval of 200 ms) and constitute the contextual information (we call them entrainers). After a longer interval (inter-stimulus interval of 600 ms), a fifth gabor patch (target) was presented and participants had to perform a task on this. The entrainers had an intermediate number of cycles per degree (cpd) of visual angle: participants had to detect if the target had an either higher or a lower cpd with respect to the entrainers. Prediction, however, was focused on a different feature of the stimuli. In fact, the gabor orientation always varied across the five visual stimuli (entrainers and target) but could either vary randomly or change gradually the orientation (clockwise or counterclockwise). In the latter case, the orientation of the target was predictable. This design nicely drives the attention of the participants on the cpd feature of the gabor patches, while manipulating the orientation for estimating the predictive processes that are supposed to be automatic. The design includes a temporal prediction dimension as well: the time gap (inter-stimulus interval) before the target gabor could be predictable (fixed time gap) or could be unpredictable (random time gap between 70 -330 miliseconds). The inclusion of this dimension makes the design predictable and non-predictable in the two dimensions (predicting what and predicting when) :

|  |  |  |
| --- | --- | --- |
|  | Predictable gabor orientation | Unpredictable gabor orientation |
| Predictable time gap (Inter stimulus interval ISI) | Predictable Orientation, Predictable Timing  (WHAT + WHEN) | Unpredictable Orientation, Predictable Timing  (WHEN Only ) |
| Unpredictable time gap  (Inter stimulus interval ISI) | Predictable Orientation, unpredictable Timing  (WHAT Only) | Unpredictable Orientation, Unpredictable Timing  (Random / None ) |

Table 1: Experimental design

Total of 160 trials were acquired for each condition (80 horizonatal target and 80 vertical target) leading to a total of 640 trials per participant. 40 trials of Functional localizers of both horizontal and vertical target were also acquired during the experiment.

The table 1 shows the four different conditions . The experimental paradigm used to generate the above mentioned four conditions is shown in figure 1:

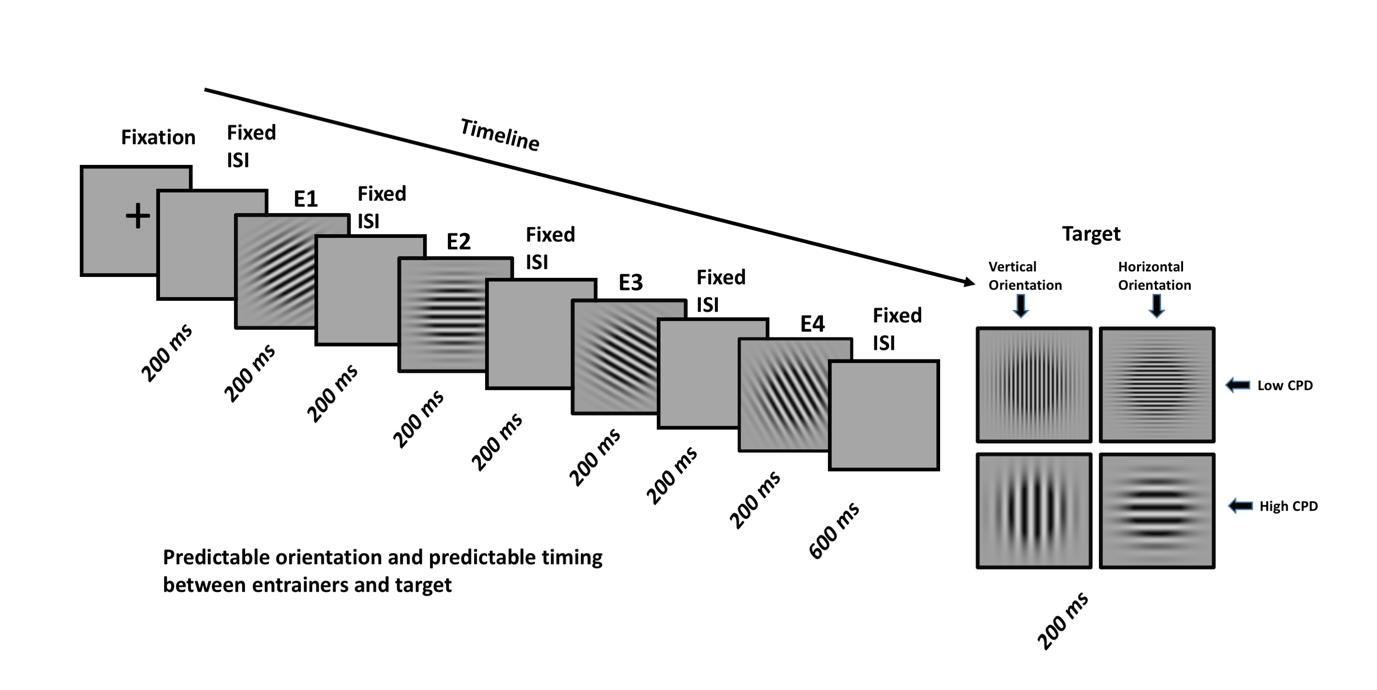


Figure 1a : Predictable orientation and predictable timing (What + When information)

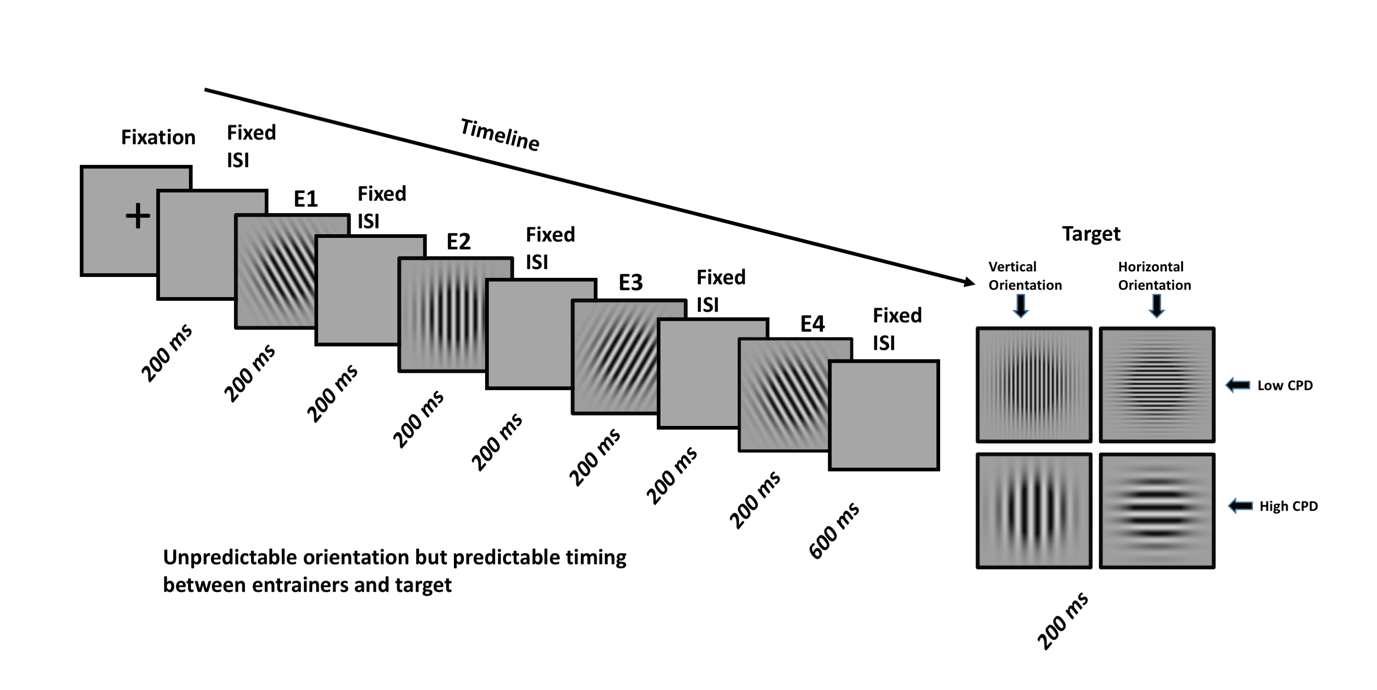


Figure 1b : Unpredictable orientation but predictable timing (When Only information)

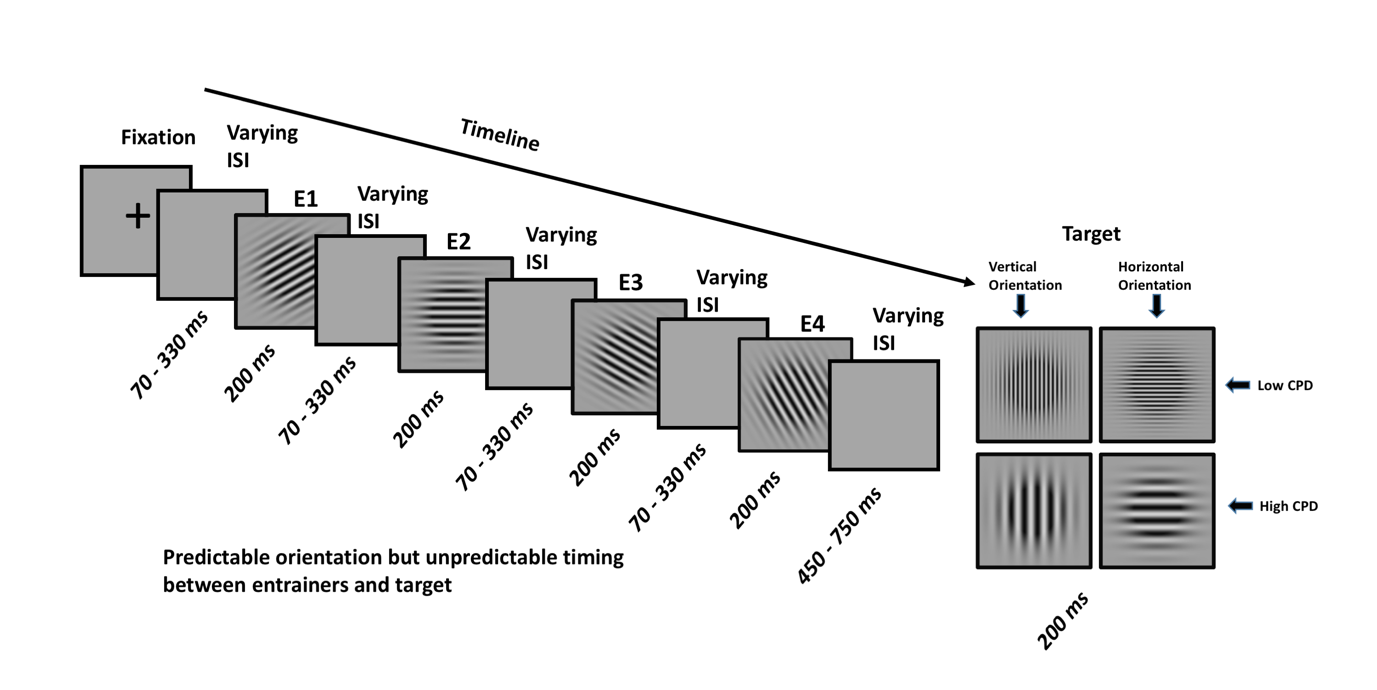


Figure 1c : Predictable orientation but unpredictable timing (What Only information)

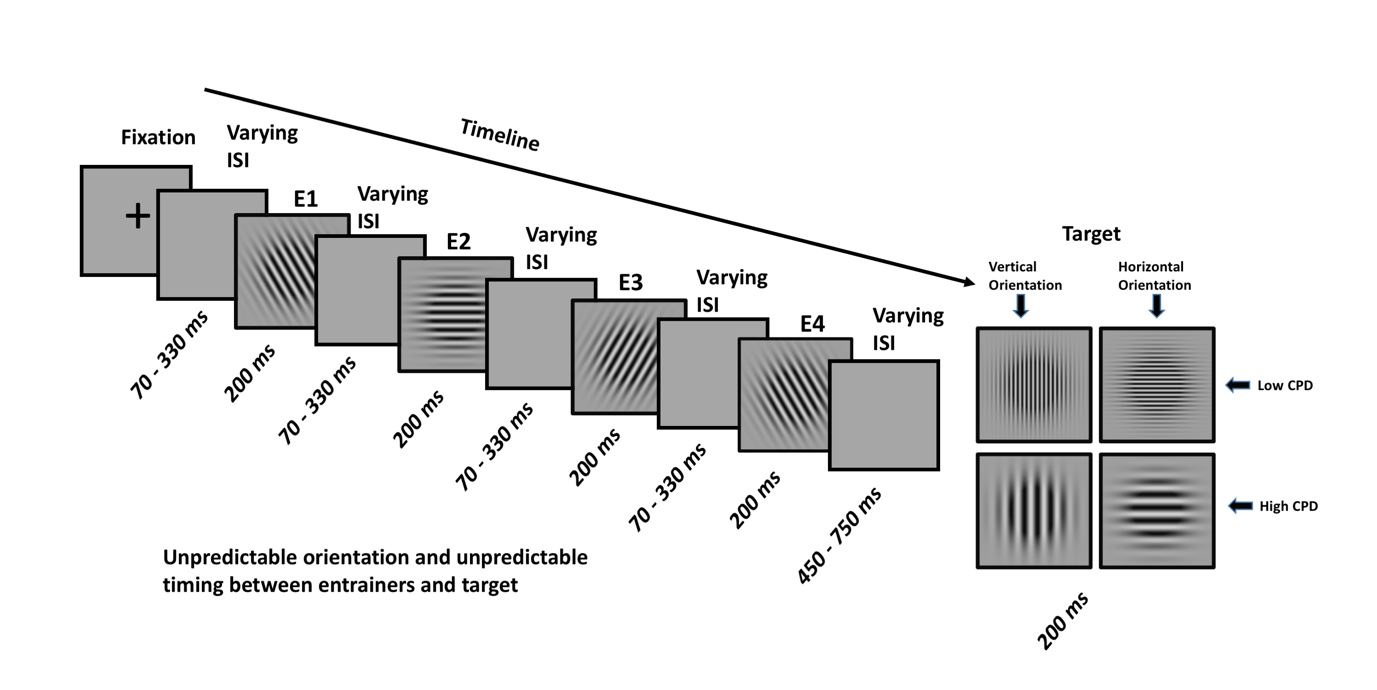


Figure 1d : Unpredictable orientation and unpredictable timing (Random/None information)

**Data Acquisition :**

MEG data were acquired using MEG facility available at Basque Center on Cognition, brain and Language (BCBL, San Sebastian, Spain) in a magnetically shielded room using the whole-scalp MEG system(Elekta NeuromagR©, Helsinki, Finland). The MEG system is equipped with 306 sensors distributed around the participant’s head. The sensors are arranged in triplet configuration of one magnetometer and two orthogonal planar gradiometers. To keep a track of head movement five (05) magnetic head position indicator (HPI) coils were also placed around the head. The initial location of the hpi coils and the three reference points i.e nasion, right auricular point and left auricular point was obtained by a 3D digitizer (Polhemus Fastrak, Colchester, VA, USA). This initial and reference point information is crucial in head motion correction during max filtering. Three hundred ( 300) additional points of the scalp of participant’s head were also obtained which helps in better coregistration of the MRI T1 images of each participant acquired at the MRI facility available at BCBL. The MRI data were acquired using a three tesla (3T) MRI machine (3T MAGNETOM PRISMAfir MR, Siemens Medical System, Erlangen,Germany) with MP2RAGE mri sequence. The MEG data was acquired at 1kz sampling rate with bandpass filter in range 0.1 to 330 Hz. Cardiac artifacts (ECG) and ocular artifacts (EOG, both blinks and saccades) were also recorded during the acquisition.

**Data preprocessing :**

The initial preprocessing were performed using maxfilter software (Maxfilter 2.2). The Spatiotemporal signal space separation (tsss) [23] along with movement correction was applied to the data. The bad channels were interpolated from neighbouring sensors with algorithms implemented in maxfilter software. The further preprocessing was performed using Fieldtrip toolbox [24] and custom scripts written in Matlab 2014b (Mathworks). The data was corrected for jump artifacts and muscle artifacts. The ocular and cardiac artifacts were automatically removed using ICA (runica) and coherence based method available on fieldtrip website.

**Evoked Analysis :**

The raw data were bandpassed in the range 0.5 - 45 hz for permorming an evoked response analysis. The planar gradiometers were combined resulting 102 channels which were used for subsequent analysis. The data was epoched based on the trigger for every entrainer. Based on the trigger values, the trials were averaged for each participant for a better signal to noise ratio. Baseline correction was also applied to the evoked data considering 400 miliseconds data prior to the cross fixation presented at beginning of each trials. Statistical difference were computed non parametric permutation test and the corrected for multiple comparisons using cluster based technique [25].

Source Reconstruction :

Source reconstruction was performed on evoked data to find out the brain areas generating the differential effect on sensor space. The source reconstruction pipeline used here has also been reported in previous work from the same group [26]. Linearly constrained minimum variance beamformer (LCMVB)[27] approach was used for creating spatial filter. T1 weighted high resolution images from 14 participants ( three participants did not perform the MRI session) were parcellated using freesurfer software[28][29]. The MEG and MRI coordinates were co-registered based on three fiducial points and marker points on brain scalp acquired during the head digitization. One shell realistic head model were created from the parcellated MRI data. The forward model was computed for three orthogonal source orientations, placed on a 5 mm grid covering the whole brain using MNE suite [30] (Martinos Centre for Biomedical Imaging). Each source was then reduced to its two principal components of highest singular value, which closely correspond to sources tangential to the skull. Both planar gradiometers and magnetometers were used for inverse modelling after dividing each sensor signal (and the corresponding forward-model coefficients) by its noise standard deviation. The noise variance was estimated from the 400 ms baseline prior to the cross fixation in every trial.

A-priori time windows based in sensor space data was selected for each entrainer (85 – 125 msec post presentation of the gabor ). LCMV inverse solution was used to project the ERF data into source space, using a noise co-variance matrix estimated from a 400 ms before the cross fixation. Source power in the selected time window was averaged and normalized by the power in the baseline. For computing the group level analysis, the individual MRIs were mapped to the standard Montreal Neurological Institute (MNI) brain through a non-linear transformation using the spatial-normalization algorithm implemented in Statistical Parametric Mapping (SPM8) [31], and the ensuing spatial transformations were applied to individual maps. We identified the coordinates of local maxima (sets of contiguous voxels displaying higher power than all other neighboring voxels). The SPM coordinates were then transformed into freesurfer coordinates and the source activity was plotted using TKsurfer tool available in freesurfer software .

Statistical inferences were computed using non parametric test and finding out the local maxima in the group maps.

MVPA:

To decode the feature specificity (i.e orientation of gabor), the data was segemented at every entrainer in time range -100 msec till 350 post presentation of gabor for Entrainer 1 , 2 and 3. Since the time gap between target and Entrainer was more compared to earlier entrainers, the data was segmented from -100 msec till 600 msec post presentation of the gabor patch. The data was classified using a linear support vector machine (SVM) classifier with L2 regularization and a box constraint of c=1. The classifier was implemented in Matlab using LibLinear [32] and the Statistics and Machine Learning Toolbox (Mathworks, Inc.). We performed a binary classification on orientation of gabor relative to the target. The label to the two classes i.e horizontal or vertical were derived from the target orientation, if the target orientation was horizontal all the preceding orientation in corresponding condition were labelled as horizontal and the other way around.

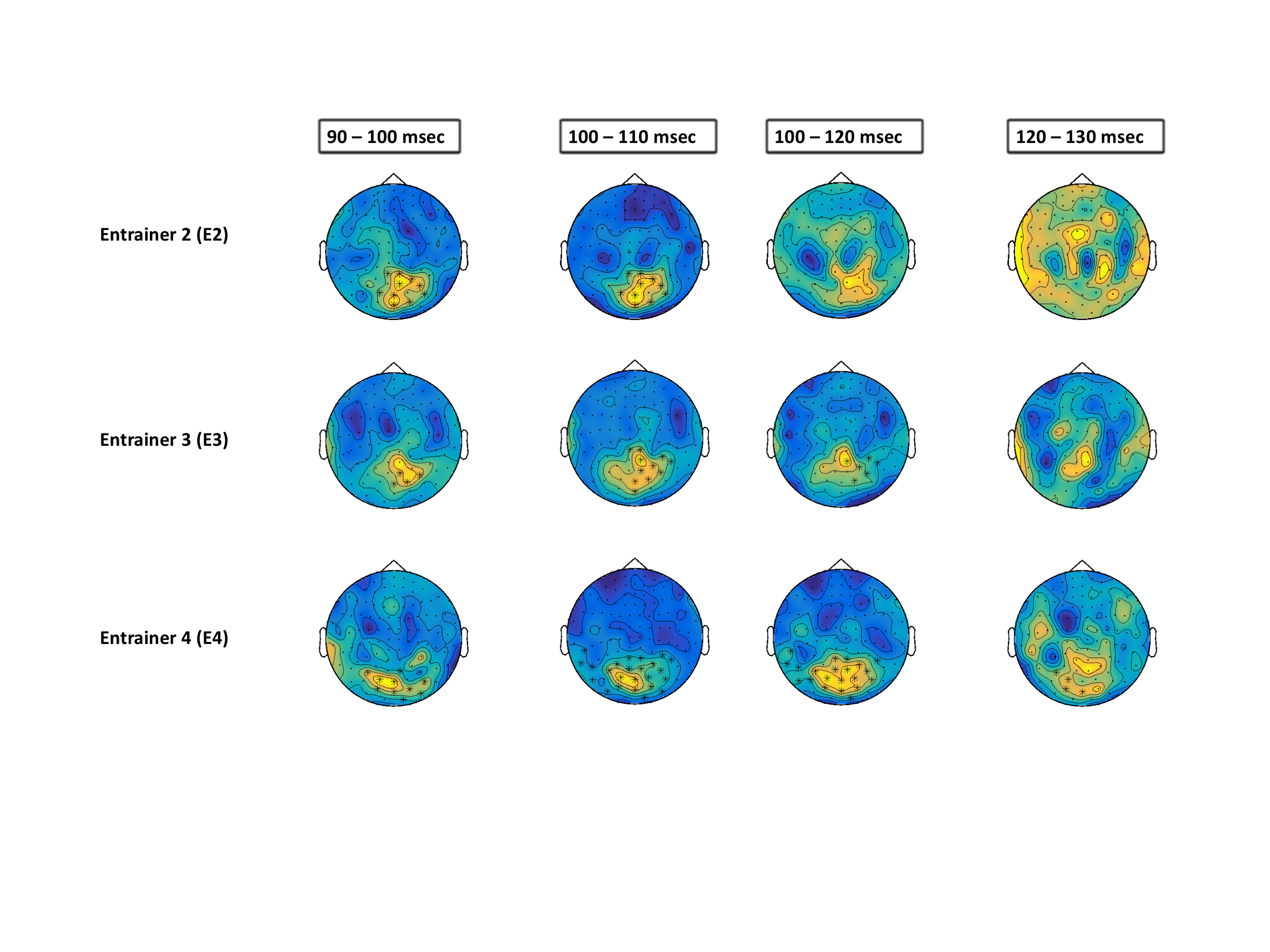
To reduce the computational load the data was down-sampled to 200 hz. Pseudo trials were generated to improve the SNR by averaging the trials in a set of 5 for each class [33]. This pseudo trial generation was repeated 100 times to generate the trials with higher signal to noise ratio. The data was then randomly partitioned using k-fold cross validation (k=5). The classifier was trained on 4 folds and tested on 1 fold and this process was repeated for all the folds. This random assignment was performed 5 times to remove any data biasness. To improve data quality, we performed multivariate noise normalization[34]. The time-resolved error covariance between sensors was calculated based on the covariance matrix (Σ) of the training set (X) and used to normalize both the training and test sets, in order to down weight MEG channels with higher noise levels.

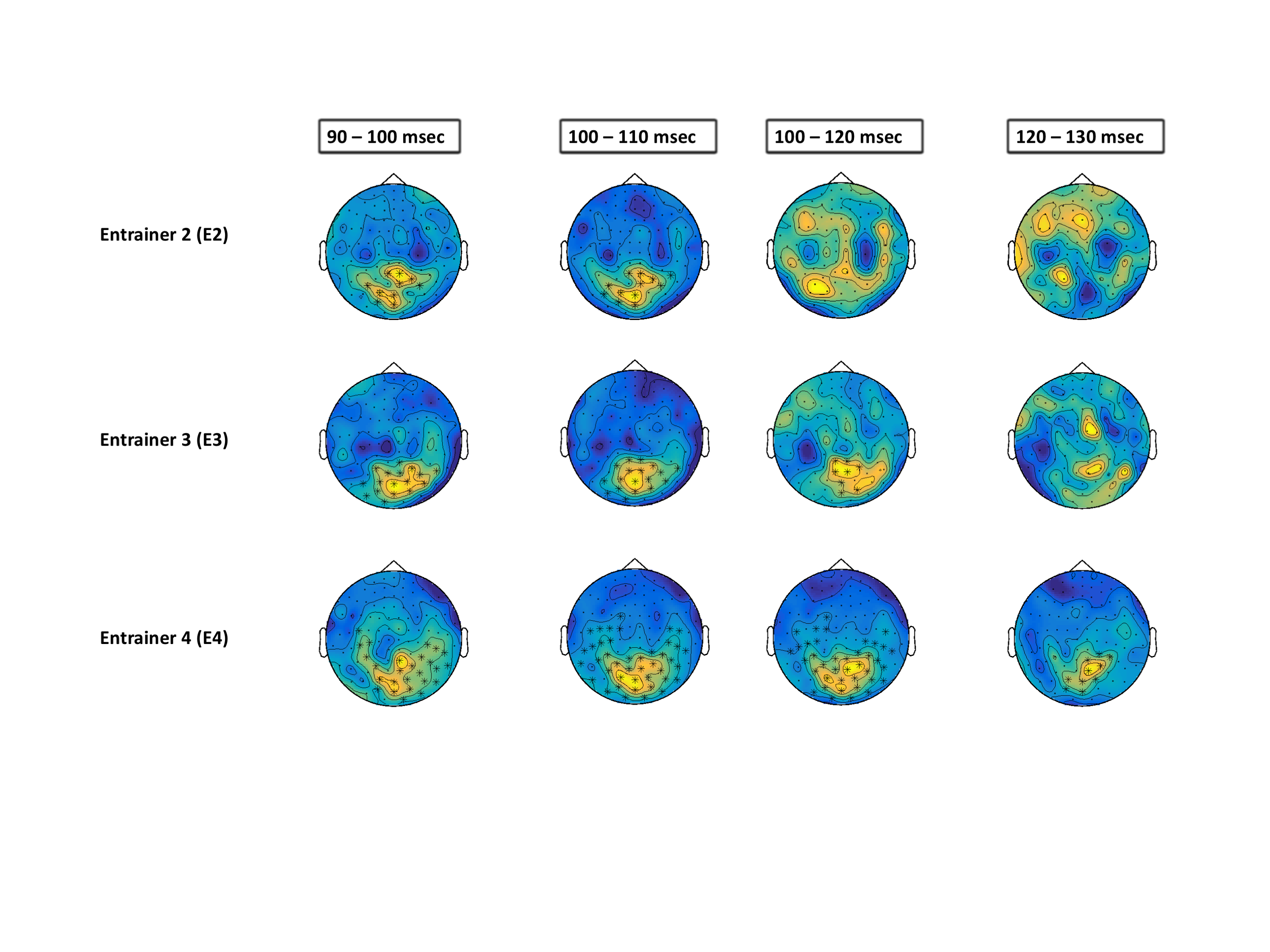
Results :

To address the experimental question, “How does the temporal predictability affect the development of predictions”, cluster based permutation test was applied to evoked data corresponding to every entrainer (E1,E2,E3 and E4). The common baseline was selected for all the conditions and entrainers i.e 400 hundred miliseconds before the cross fixation in the data. Table 2 contains the output of cluster based permutation test between conditons at every entrainer. The alpha threshold was considered as 0.01 and time window for cluster based permutation test was selected from 0 – 270 msec with 1000 random permutations . To access the strong and localised clusters during correction, the clusteralpha parameter was also set to 0.01.

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
|  | Entrainer 1 | Entrainer 2 | Entrainer 3 | Entrainer 4 |
| What + When  Vs  When Only | No Significant Differences | 95 – 105 msec (p< 0.01) | 96 – 110 msec  (p< 0.001) | 97 – 121 msec  (p<0.001) |
| When Only  Vs  None/Random | No Significant Differences | 95 – 109 msec (p< 0.001) | 94 – 113 msec  (p< 0.001) | 96 – 129 msec  (p<0.001) |

Figure 2 shows the topographic information of differences along with the highlighted channels below threshold,



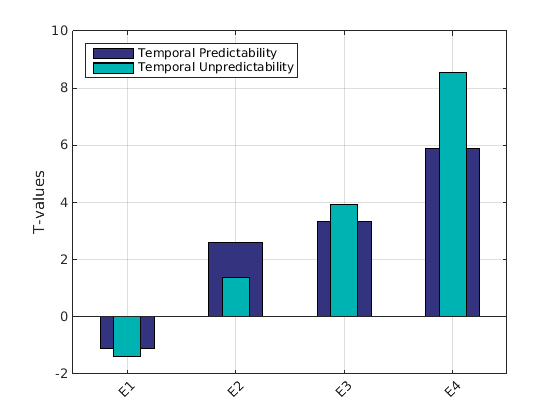


**Source Reconstruction :**

The evoked analysis shows that there are significant differences between condition which starts from entrainer 2 and the effect goes stronger as we move ahead in time. The no of channels involved in the difference is also increase which refers to the higher differences across conditions. The local maxima were computed within every condition. Table 2 shows the significant local maxima obtained in every group map at every entrainer.

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
|  | E 1 | E2 | E3 | E4 |
| What + When | -1 -92 -12 | -1 -89 -15  19 -95 12 | 1 -90 -14  22 -95 12 | 0 -91 -12 |
| When Only | -1 -93  -9 | -1 -90 -14  20 -95 13 | 0 -91 -13  22 -95 14 | 0 -91 -13  22 -95 -13 |
| What only | -2 -93 -9 | -2 -89 -16  22 -95 12 | 0 -90 -14  22 -95 11 | -1 -92 -10 |
| None / Random | -2 -93 -9 | 0 -91 -13  18 -94 14 | 1 -91 -13  21 -95 12 | 0 -92 -11  21 -95 13 |

The first MNI coordinate [-1 -91 -12] was considered for further analysis, considering the spatial resolution of MEG and the spectral leakage limitation in the inverse operation methods, all the local maxima within few mm of the first maxima are supposed to have same neural source. Taking the MNI coordinate [-1 -92 -12] as center a sphere having 5mm diameter was drawn in the MNI space. The maximum source activity within this sphere was calculated for every participant. To find out if mean of groups come from a same or different distribution, one sample dependent ttest was applied to the power ratio values across conditions. Figure 3 shows the t-values compared between conditions having temporable predictability (i.e *What + When vs When Only* ) and without temporable predictability (i.e *What only vs None*).



It is evident from the tvalue differences that conditions having temporable predictability are processed faster in time (i.e the differences start at E2) whereas the conditions lacking temporable predictability are processed later but then the differences becomes stronger compared to conditions having temporable predictability. Figure 4 shows the mean of power ratios at every condition across entrainers.

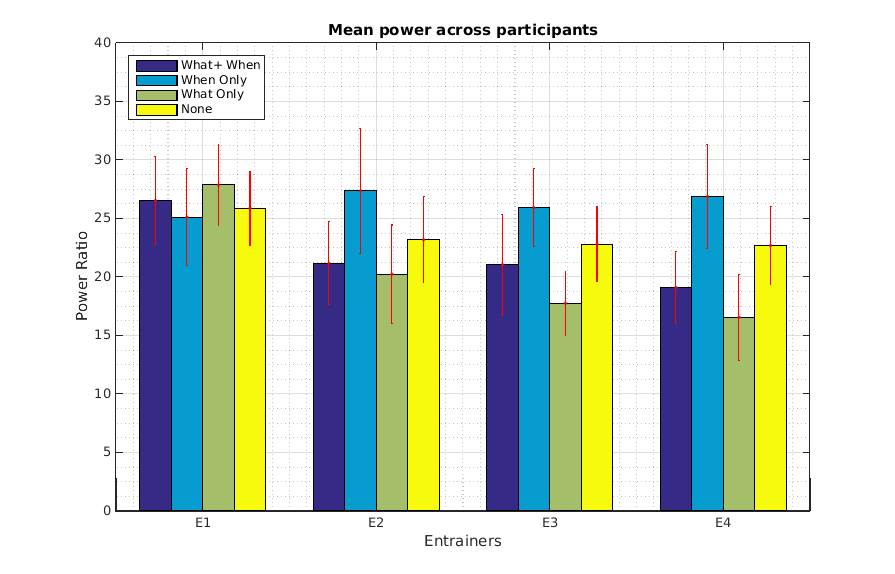
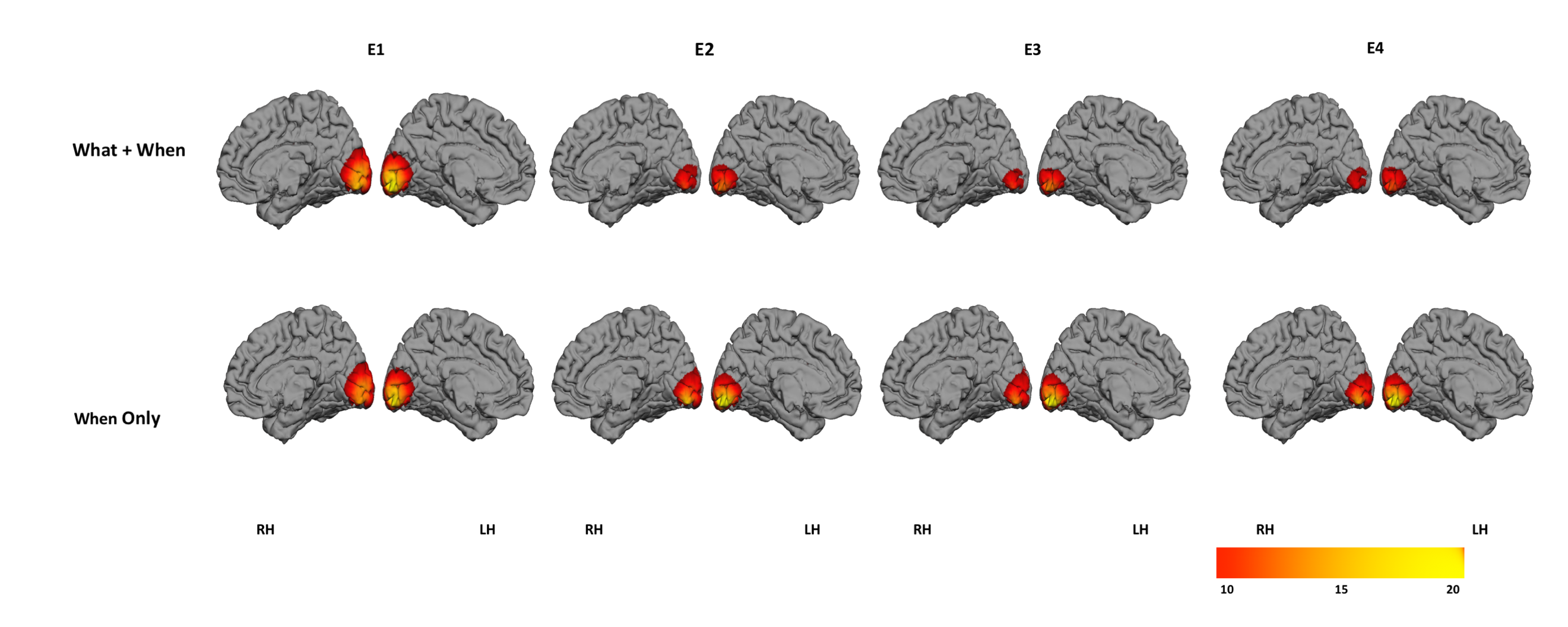
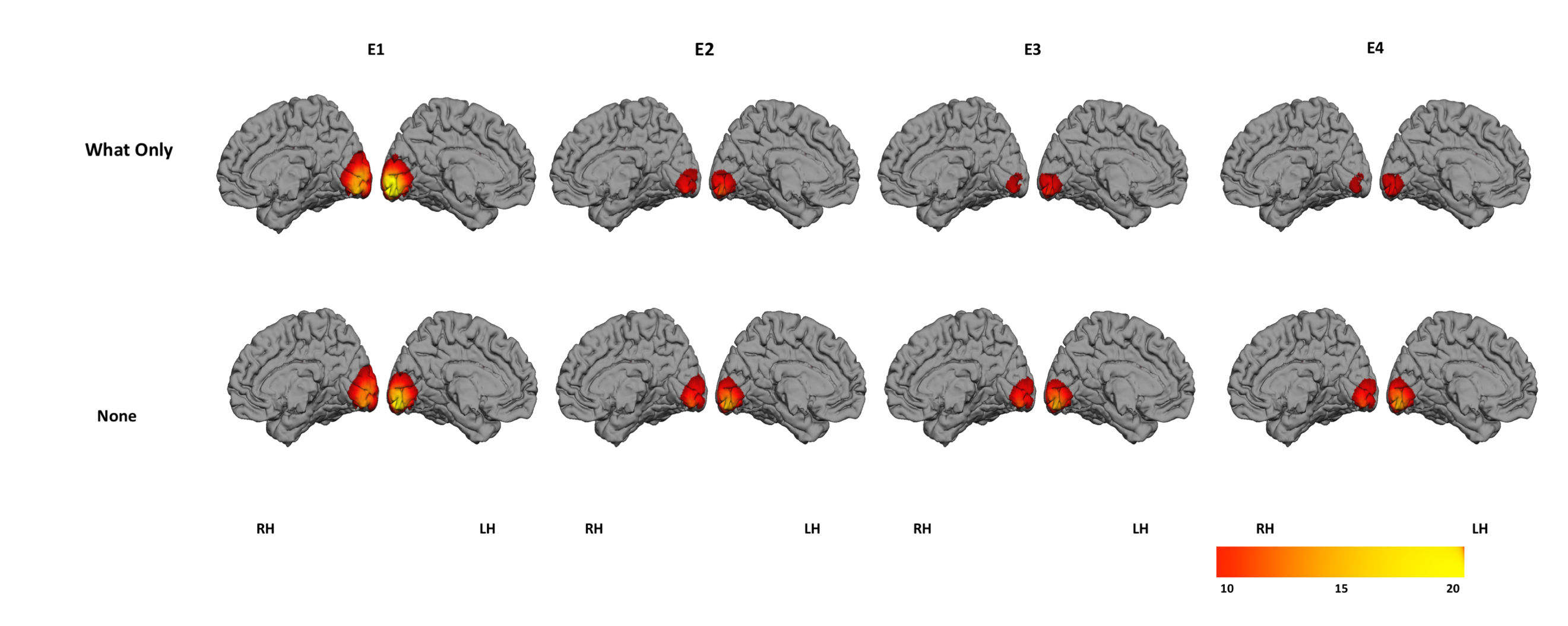


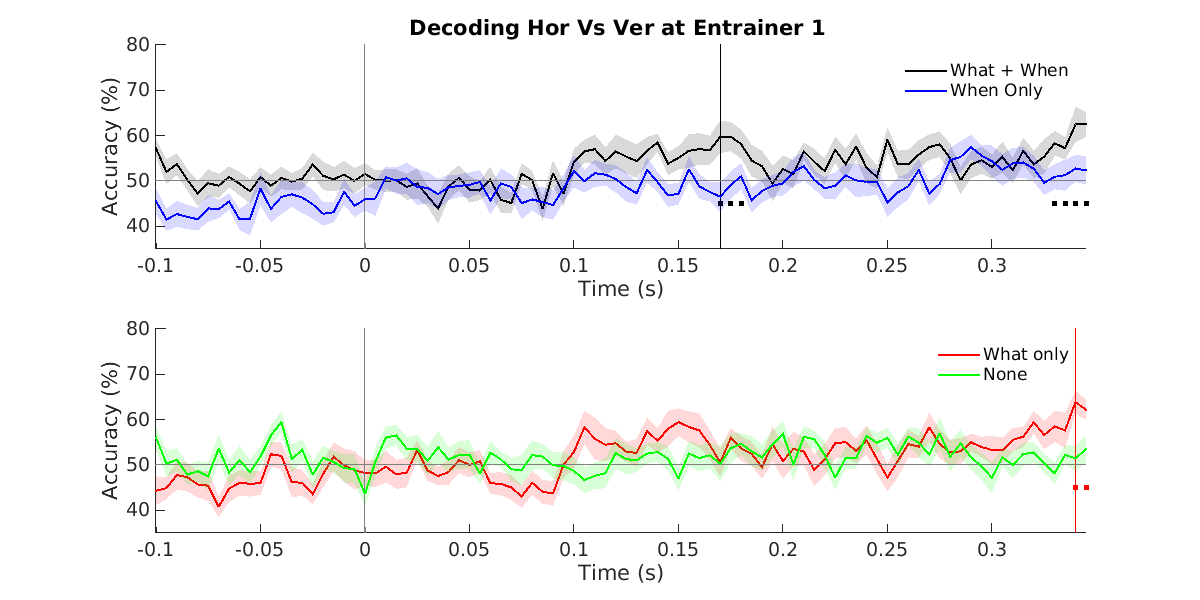
Figure 5 shows the group activity of the conditions with and without temporal predictability. It is evident that the conditions having predictable orientation (i.e *What + When and When Only)* shows reduction in the neural activity as we move across the entrainers, whereas the conditions without the orientation predictability does not show such reduction.

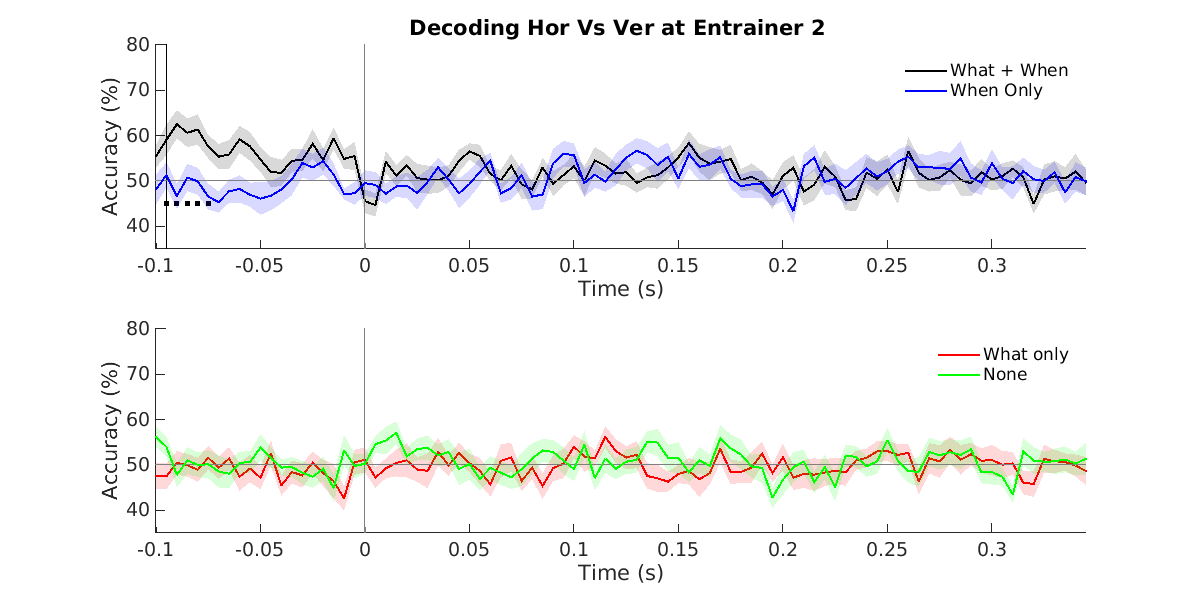
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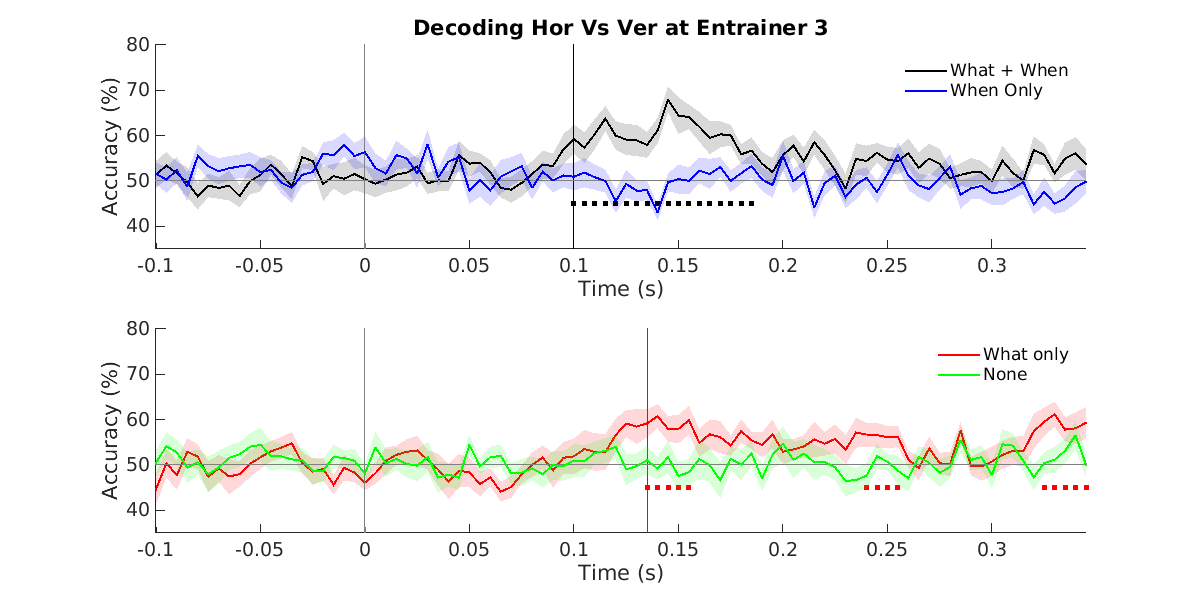


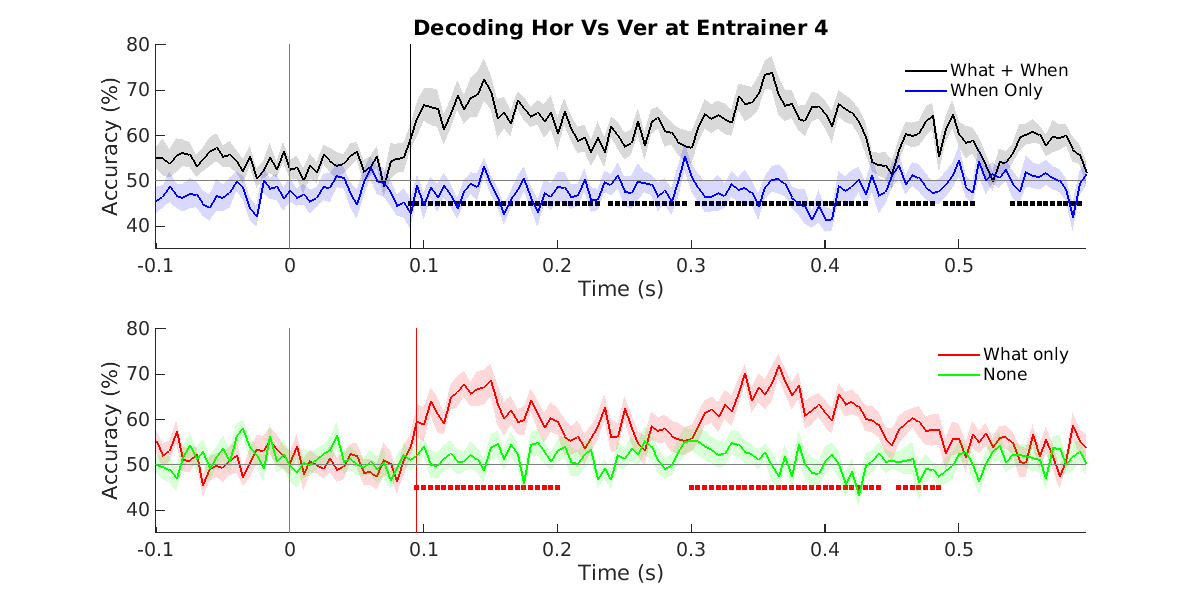
**MVPA results :**

The data was time locked to each entrainer in a time range of -100 msec to 350 msec (will change it ) post presentation of the gabor for entrainer 1 to entrainer 3. Since the entrainer 4 has a longer time gap between the entrainer and target so data was selected from -100 to 600 msec post presentation of gabor. Each trial was labelled as horizontal or vertical relative to the target. For example a trial was labelled Horizontal if the target i.e fifth gabor patch has a horizontal orientation angle of the gabor patch. Figure 6 shows the decoding of horizontal versus vertical target at every entrainer.









It can be inferred from figure 5 that decoding of the orientation is not decodable at entrainer 1 (E1) in all the four conditions. The same holds true for entrainer 2. As the time progress to entrainer 3, the conditions having the information about the orientation (i.e *What + When and What only*) shows above chance and statistically significant decoding accuracy. At entrainer 3, the significant decoding starts around ~ 90 miliseconds in condition having temporable predictability, whereas the condition lacking temporable predictability starts around ~ 135 miliseconds. The decoding is also consistent in condition having temporable predictability whereas the condition lacking temporable predictability is recurrent in nature. At Entrainer 4, the difference between the first decoding point is almost similar whereas the decoding of orientation is constant for a longer time in condition having temporal predictability (i.e *What + When* ) compared to the condition lacking temporable predictability (i.e *What Only* ). It is also worth noticing the conditions which don’t have the information about the orientation of the gabor patch (i.e *When only and None* ) , the decoding accuracy is always around chance which reflects the effectiveness of the classifier used.

**Discussion :**

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Declaration : The **author**(s) **declare**(s) that there is **no conflict of interest** regarding the publication of this article.

**References :**

[1] G. B. Keller and T. D. Mrsic-Flogel, “Predictive Processing: A Canonical Cortical Computation,” *Neuron*, vol. 100, no. 2, pp. 424–435, 2018.

[2] K. Friston, “A theory of cortical responses,” *Philos. Trans. R. Soc. B Biol. Sci.*, vol. 360, no. 1456, pp. 815–836, 2005.

[3] R. P. N. Rao and D. H. Ballard, “Predictive coding in the visual cortex: A functional interpretation of some extra-classical receptive-field effects,” *Nat. Neurosci.*, vol. 2, no. 1, pp. 79–87, 1999.

[4] C. G. Richter, W. H. Thompson, C. A. Bosman, and P. Fries, “Top-down beta enhances bottom-up gamma,” *J. Neurosci.*, vol. 37, no. 28, pp. 6698–6711, 2017.

[5] G. Stefanics, G. Stefanics, J. Kremláček, and I. Czigler, “Visual mismatch negativity: A predictive coding view,” *Front. Hum. Neurosci.*, vol. 8, no. September, pp. 1–19, 2014.

[6] L. H. Arnal and A. L. Giraud, “Cortical oscillations and sensory predictions,” *Trends Cogn. Sci.*, vol. 16, no. 7, pp. 390–398, 2012.

[7] M. Heilbron and M. Chait, “Great Expectations: Is there Evidence for Predictive Coding in Auditory Cortex?,” *Neuroscience*, vol. 389, pp. 54–73, 2018.

[8] M. Hakonen, P. J. C. May, I. P. Jääskeläinen, E. Jokinen, M. Sams, and H. Tiitinen, “Predictive processing increases intelligibility of acoustically distorted speech: Behavioral and neural correlates,” *Brain Behav.*, vol. 7, no. 9, pp. 1–15, 2017.

[9] Gina R. Kuperberg and T. F. Jaeger, “What do we mean by prediction in language comprehension?,” *Physiol. Behav.*, vol. 176, no. 3, pp. 139–148, 2017.

[10] S. Koelsch, P. Vuust, and K. Friston, “Predictive Processes and the Peculiar Case of Music,” *Trends Cogn. Sci.*, vol. 23, no. 1, pp. 63–77, 2019.

[11] P. Sinha *et al.*, “Autism as a disorder of prediction,” *Proc. Natl. Acad. Sci. U. S. A.*, vol. 111, no. 42, pp. 15220–15225, 2014.

[12] P. Sterzer *et al.*, “The Predictive Coding Account of Psychosis,” *Biol. Psychiatry*, vol. 84, no. 9, pp. 634–643, 2018.

[13] J. Costa-Faidella, T. Baldeweg, S. Grimm, and C. Escera, “Interactions between ‘what’ and ‘when’ in the auditory system: Temporal predictability enhances repetition suppression,” *J. Neurosci.*, vol. 31, no. 50, pp. 18590–18597, 2011.

[14] R. Auksztulewicz *et al.*, “Not all predictions are equal: ‘what’ and ‘when’ predictions modulate activity in auditory cortex through different mechanisms,” *J. Neurosci.*, vol. 38, no. 40, pp. 8680–8693, 2018.

[15] E. B. V All and W. James, “Bridging prediction and attention in current research on perception and action,” vol. 1626, pp. 1–13, 2015.

[16] X. V. Wyart, N. E. Myers, and C. Summerfield, “Neural Mechanisms of Human Perceptual Choice Under Focused and Divided Attention,” vol. 35, no. 8, pp. 3485–3498, 2015.

[17] C. Summerfield and J. A. Mangels, “Dissociable Neural Mechanisms for Encoding Predictable and Unpredictable Events,” pp. 1120–1132, 2006.

[18] J. Jiang, C. Summerfield, and T. Egner, “Attention Sharpens the Distinction between Expected and Unexpected Percepts in the Visual Brain,” vol. 33, no. 47, pp. 18438–18447, 2013.

[19] K. Grill-Spector, R. Henson, and A. Martin, “Repetition and the brain: Neural models of stimulus-specific effects,” *Trends Cogn. Sci.*, vol. 10, no. 1, pp. 14–23, 2006.

[20] J. R. King, N. Pescetelli, and S. Dehaene, “Brain Mechanisms Underlying the Brief Maintenance of Seen and Unseen Sensory Information,” *Neuron*, vol. 92, no. 5, pp. 1122–1134, 2016.

[21] D. Pantazis, M. Fang, S. Qin, Y. Mohsenzadeh, Q. Li, and R. M. Cichy, “Decoding the orientation of contrast edges from MEG evoked and induced responses,” *Neuroimage*, vol. 180, no. July, pp. 267–279, 2018.

[22] R. M. Cichy, D. Pantazis, and A. Oliva, “Resolving human object recognition in space and time,” *Nat. Neurosci.*, vol. 17, no. 3, pp. 455–462, 2014.

[23] S. Taulu and J. Simola, “Spatiotemporal signal space separation method for rejecting nearby interference in MEG measurements,” *Phys. Med. Biol.*, vol. 51, no. 7, pp. 1759–1768, 2006.

[24] R. Oostenveld, P. Fries, E. Maris, and J. M. Schoffelen, “FieldTrip: Open source software for advanced analysis of MEG, EEG, and invasive electrophysiological data,” *Comput. Intell. Neurosci.*, vol. 2011, 2011.

[25] E. Maris and R. Oostenveld, “Nonparametric statistical testing of EEG- and MEG-data,” *J. Neurosci. Methods*, vol. 164, no. 1, pp. 177–190, 2007.

[26] I. F. Monsalve, M. Bourguignon, and N. Molinaro, “Theta oscillations mediate pre-activation of highly expected word initial phonemes,” *Sci. Rep.*, vol. 8, no. 1, pp. 1–14, 2018.

[27] B. D. Van Veen, W. Van Drongelen, M. Yuchtman, and A. Suzuki, “Localization of brain electrical activity via linearly constrained minimum variance spatial filtering. IEEE Transactions on,” *Biomed. Eng. (NY).*, vol. 44, no. 9, pp. 867–880, 1997.

[28] A. M. Dale, B. Fischl, and M. I. Sereno, “Cortical Surface-Based Analysis,” *Neuroimage*, vol. 9, no. 2, pp. 179–194, 1999.

[29] A. Dale and M. Sereno, “Improved localization of cortical surface reconstruciton: A linear approach.,” *J. Cogn. Neurosci.*, vol. 5, pp. 162–176, 1993.

[30] A. Gramfort *et al.*, “MNE software for processing MEG and EEG data,” *Neuroimage*, vol. 86, pp. 446–460, 2014.

[31] K. J. Friston, A. P. Holmes, K. J. Worsley, J. ‐P Poline, C. D. Frith, and R. S. J. Frackowiak, “Statistical parametric maps in functional imaging: A general linear approach,” *Hum. Brain Mapp.*, vol. 2, no. 4, pp. 189–210, 1994.

[32] R. E. Fan, K. W. Chang, C. J. Hsieh, X. R. Wang, and C. J. Lin, “LIBLINEAR: A library for large linear classification,” *J. Mach. Learn. Res.*, vol. 9, no. 2008, pp. 1871–1874, 2008.

[33] D. C. Dima and K. D. Singh, “Dynamic representations of faces in the human ventral visual stream link visual features to behaviour,” 2018.

[34] M. Guggenmos, P. Sterzer, and R. M. Cichy, “Multivariate pattern analysis for MEG: A comparison of dissimilarity measures,” *Neuroimage*, vol. 173, no. February, pp. 434–447, 2018.

**Supplementary Data :**

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
|  | E1 | E2 | E3 | E4 |
| Cond\_2 vs Cond\_1 | -1.118 | 2.6157 | 3.335 | 5.8860 |
| Cond\_4 vs  Cond\_3 | -1.387 | 1.3875 | 3.9145 | 8.5556 |

Table a