

Recommendations for Cardiac Chamber Quantification by Echocardiography in Adults: An Update from the American Society of Echocardiography and the European Association of Cardiovascular Imaging

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The rapid technological developments of the past decade and the changes in echocardiographic practice brought about by these developments have resulted in the need for updated recommendations to the previously published guidelines for cardiac chamber quantification, which was the goal of the joint writing group assembled by the American Society of Echocardiography and the European Association of Cardiovascular Imaging. This document provides updated normal values for all four cardiac chambers, including three-dimensional echocardiography and myocardial deformation, when possible, on the basis of considerably larger numbers of normal subjects, compiled from multiple databases. In addition, this document attempts to eliminate several minor discrepancies that existed between previously published guidelines.

Keywords Adult echocardiography • Transthoracic echocardiography • Ventricular function • Normal values

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The quantification of cardiac chamber size and function is the cornerstone of cardiac imaging, with echocardiography being the most commonly used noninvasive modality because of its unique ability to provide real-time images of the beating heart, combined with its availability and portability. Standardization of the methodology used to quantify cardiac chambers is maintained by creating and disseminating official recommendations, which when followed by practitioners provides uniformity and facilitates communication. Recommendations for echocardiographic chamber quantification were last published in 2005 by the American Society of Echocardiography (ASE) and the European Association of Echocardiography (renamed the European Association of Cardiovascular Imaging [EACVI]).^{1,2}

Since then, echocardiographic technology has continued evolving, with two major developments being real-time three-dimensional (3D) echocardiography (3DE) and myocardial deformation imaging. The goal of this document is to provide an update to the previously published guidelines, as well as recommendations and reference values, while eliminating the minor discrepancies that existed between previous guidelines. The normal values in this update include 3DE and myocardial deformation, when possible. Importantly, compared with the previous guidelines, this update is based on considerably larger numbers of normal subjects, compiled from multiple databases, to improve the reliability of the reference values.

Although most issues covered in this document reflect a broad consensus among the members of the writing group, one important issue the group debated was partition values for severity of abnormalities. Most often, in addition to describing a parameter as normal or abnormal (reference values), clinical echocardiographers qualify the degree of abnormality with terms such as *mildly*, *moderately*, and *severely abnormal*, which reflect the degree to which measurements deviate from normal. In addition to providing normative data, it would be beneficial to standardize cutoffs for severity of abnormality for all parameters across echocardiography laboratories, such that the term *moderately abnormal*, for example, would have the same meaning universally. However, different approaches may be used for determining cutoff values for the different degrees of abnormality, all of which have significant limitations.

The first approach would be to empirically define cutoffs for mild, moderate, and severe abnormalities on the basis of SDs above or below the reference limit derived from a group of healthy people. The advantage of this method is that these data readily exist for most echocardiographic parameters. However, this approach is fundamentally flawed. First, not all echocardiographic parameters are normally distributed (or Gaussian), even in a normal population.

Second, even if a particular parameter is normally distributed in normal subjects, most echocardiographic parameters, when measured in the general population, have a significant asymmetric distribution in one direction (abnormally large for size or abnormally low for function parameters). An alternative method would be to define abnormalities on the basis of percentile values (e.g., 95th, 99th) of measurements derived from a population that includes both healthy people and those with disease. Although these data would still not be normally distributed, they would account for the asymmetric distribution and the range of abnormality present within the general population. The major limitation of this approach is that such population data sets simply do not exist for most echocardiographic variables.

Ideally, an approach that predicts outcomes or prognosis would be preferred. That is, defining a variable as moderately deviated from normal would imply that there is a moderate risk for a particular adverse outcome for a patient. Although sufficient data linking risk and cardiac chamber sizes exist for several parameters (e.g., left ventricular [LV] size and ejection fraction [EF], left atrial [LA] volume), outcomes data are lacking for many other parameters. Unfortunately, this approach also has limitations. The first obstacle is how to best define risk. The cutoffs suggested for the same parameter vary broadly for different risks in different patient populations and disease states.

Last, cutoff values may be determined by experience-based consensus of expert opinions. An extensive debate arose among the members of the writing group, some of whom felt that providing partition values on the basis of this scientifically less-than-rigorous approach would be a disservice to the echocardiography community and that a disease-specific approach might be required to achieve meaningful clinical categorization of the severity of abnormality. Others felt that such cutoffs would provide a uniform reference for echocardiographic reporting, which would be easier to interpret by referring clinicians. The compromise was to provide experience-based partition values only for LV EF and LA volume, while suggested partition values for additional parameters of LV size and mass are listed in the Appendix. All partition values should be interpreted with caution in this perspective.

For parameters other than LV size, function, and mass as well as LA volume, only the mean value and the SD of gender-, age-, and body surface area (BSA)-normalized cutoffs or upper and lower limits are reported in the appropriate sections of this document. For these parameters, measurements exceeding ± 1.96 SDs (i.e., the 95% confidence interval) should be classified as abnormal. Any description of the degree of deviation from normality in the echocardiographic report should remain at the discretion of the individual laboratory, and the writing group does not recommend specific partition values.

Quantification using transesophageal echocardiography (TEE) has advantages and disadvantages compared with transthoracic echocardiography (TTE). Although visualization of many cardiac structures is improved with TEE, some differences in measurements have been found between TEE and TTE, particularly for chamber dimensions and thickness. These differences are primarily attributable to the inability to obtain from the transesophageal approach the standardized imaging planes and views used when quantifying chamber dimensions transthoracically. It is the recommendation of this writing group that

the same range of normal values for LV and right ventricular (RV) chamber dimensions and volumes apply for both TEE and TTE. For details on specific views for optimal measurements, please refer to the recently published TEE guidelines.³

All measurements described in this document should be performed on more than one cardiac cycle to account for interbeat variability. The committee suggests the average of three beats for patients in normal sinus rhythm and a minimum of five beats in patients with atrial fibrillation. Because the committee acknowledges that the implementation of this recommendation is time consuming, the use of representative beats is acceptable in the clinical setting.

I. The Left Ventricle

1. Measurement of LV Size

The most commonly used parameters to describe LV cavity size include linear internal dimensions and volumes. Measurements are commonly reported for end-diastole and end-systole, which are then used to derive parameters of global LV function. To allow comparison among individuals with different body sizes, chamber measurements should be reported indexed to BSA.

1.1 Linear Measurements

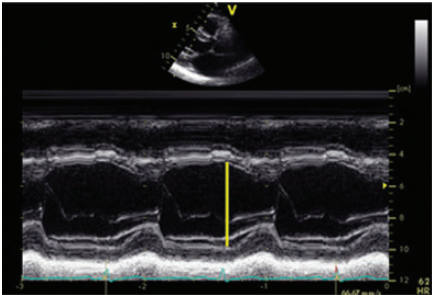
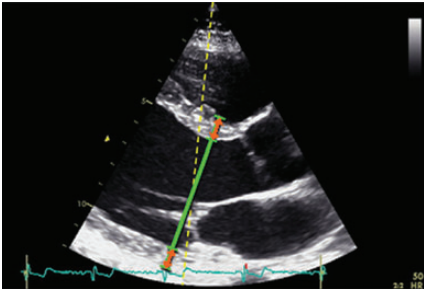
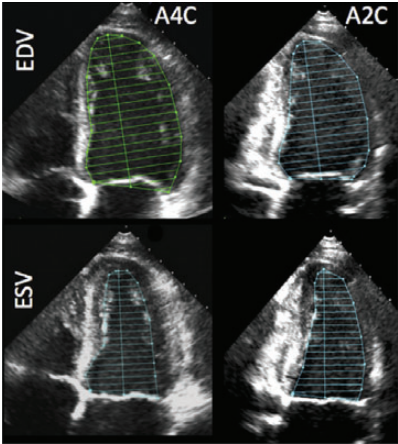
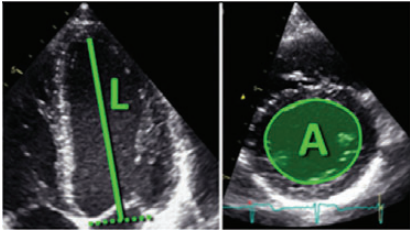
It is recommended that linear internal measurements of the left ventricle and its walls be performed in the parasternal long-axis view. Values should be carefully obtained perpendicular to the LV long axis and measured at or immediately below the level of the mitral valve leaflet tips. In this regard, the electronic calipers should be positioned on the interface between the myocardial wall and cavity and the interface between the wall and the pericardium. Internal dimensions can be obtained with a two-dimensional (2D) echocardiography (2DE)-guided M-mode approach, although linear measurements obtained from 2D echocardiographic images are preferred to avoid oblique sections of the ventricle (Table 1).

1.2 Volumetric Measurements

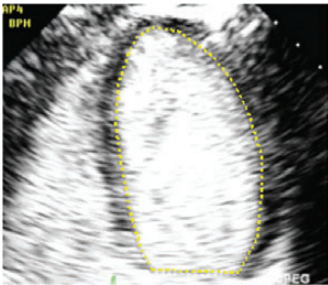
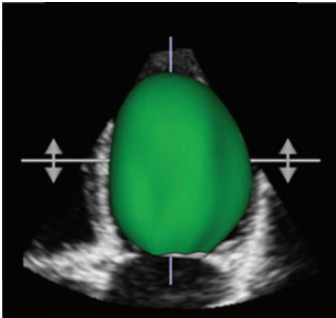
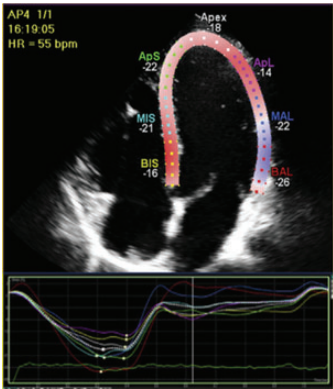
LV volumes are measured using 2DE or 3DE. Volume calculations derived from linear measurements may be inaccurate, because they rely on the assumption of a fixed geometric LV shape such as a prolate ellipsoid, which does not apply in a variety of cardiac pathologies. Accordingly, the Teichholz and Quinones methods for calculating LV volumes from LV linear dimensions are no longer recommended for clinical use.

Volumetric measurements are usually based on tracings of the interface between the compacted myocardium and the LV cavity. At the mitral valve level, the contour is closed by connecting the two opposite sections of the mitral ring with a straight line. LV length is defined as the distance between the bisector of this line and the apical point of the LV contour, which is most distant to it. The use of the longer LV length between the apical two- and four-chamber views is recommended.

LV volumes should be measured from the apical four- and two-chamber views. Two-dimensional echocardiographic image acquisition should aim to maximize LV areas, while avoiding foreshortening of the left ventricle, which results in volume underestimation. Acquiring LV views at a reduced depth to focus on the LV cavity will reduce

Parameter and method	Technique	Advantages	Limitations
Internal linear dimensions Linear internal measurements of the LV should be acquired in the parasternal long-axis view carefully obtained perpendicular to the LV long axis, and measured at the level of the mitral valve leaflet tips. Electronic calipers should be positioned on the interface between myocardial wall and cavity and the interface between wall and pericardium (orange arrows).	M-mode tracing 	<ul style="list-style-type: none">• Reproducible• High temporal resolution• Wealth of published data	<ul style="list-style-type: none">• Beam orientation frequently off axis• Single dimension, i.e., representative only in normally shaped ventricles
	2D-guided linear measurements 	<ul style="list-style-type: none">• Facilitates orientation perpendicular to the ventricular long axis	<ul style="list-style-type: none">• Lower frame rates than M-mode• Single dimension, i.e., representative only in normally shaped ventricles
Volumes Volume measurements are usually based on tracings of the blood-tissue interface in the apical four- and two-chamber views. At the mitral valve level, the contour is closed by connecting the two opposite sections of the mitral ring with a straight line. LV length is defined as the distance between the middle of this line and the most distant point of the LV contour.	Biplane disk summation 	<ul style="list-style-type: none">• Corrects for shape distortions• Less geometrical assumptions compared with linear dimensions	<ul style="list-style-type: none">• Apex frequently foreshortened• Endocardial dropout• Blind to shape distortions not visualized in the apical two- and four-chamber planes
	Area-length 	<ul style="list-style-type: none">• Partial correction for shape distortion	<ul style="list-style-type: none">• Apex frequently foreshortened• Heavily based on geometrical assumptions• Limited published data on normal population

Continued

Parameter and method	Technique	Advantages	Limitations
	Endocardial border enhancement 	<ul style="list-style-type: none">• Helpful in patients with suboptimal acoustic window• Provides volumes that are closer to those measured with cardiac magnetic resonance	<ul style="list-style-type: none">• Same limitations as the above non-contrast 2D techniques• Acoustic shadowing in LV basal segments with excess contrast
	3D data sets 	<ul style="list-style-type: none">• No geometrical assumption• Unaffected by foreshortening• More accurate and reproducible compared to other imaging modalities	<ul style="list-style-type: none">• Lower temporal resolution• Less published data on normal values• Image quality dependent
Global longitudinal strain Peak value of 2D longitudinal speckle tracking derived strain (%).		<ul style="list-style-type: none">• Angle independent• Established prognostic value	<ul style="list-style-type: none">• Vendor dependent

2D, two-dimensional; 3D, three-dimensional; A2C, apical 2-chamber view; A4C, apical 4-chamber view; EDV, end-diastolic volume; ESV, end-systolic volume; LV, left ventricular.

the likelihood of foreshortening and minimize errors in endocardial border tracings (Table 1). Because the issue of foreshortening is less relevant in 3D data sets, 3D image acquisition should focus primarily on including the entire left ventricle within the pyramidal data set. To ensure reasonably accurate identification of end-systole, the temporal resolution of 3D imaging should be maximized without compromising spatial resolution.

Contrast agents should be used when needed to improve endocardial delineation when two or more contiguous LV endocardial segments are poorly visualized in apical views, as per published guidelines.⁴ Contrast-enhanced images may provide larger volumes than unenhanced images that are closer to those obtained with cardiac magnetic resonance (CMR) in head-to-head comparison.⁵ Care

should be taken to avoid acoustic shadowing, which may occur in LV basal segments in the presence of high concentrations of contrast. Normal reference values for LV volumes with contrast enhancement are not well established.

The most commonly used method for 2D echocardiographic volume calculations is the biplane method of disks summation (modified Simpson's rule), which is the recommended 2D echocardiographic method by consensus of this committee (Table 1). An alternative method to calculate LV volumes when apical endocardial definition precludes accurate tracing is the area-length method, in which the LV is assumed to be bullet shaped. The mid-LV cross-sectional area is computed by planimetry in the parasternal short-axis view and the length of the ventricle taken from the midpoint of the

annular plane to the apex in the apical four-chamber view (Table 1). The shortcoming of this method is that the bullet-shape assumption does not always hold true. One of the advantages of 3D echocardiographic volume measurements is that they do not rely on geometric assumptions. In patients with good image quality, 3D echocardiographic measurements are accurate and reproducible and should therefore be used when available and feasible.⁶ The advantages and disadvantages of the various methods are summarized in Table 1.

1.3 Normal Reference Values for 2DE

Data were extracted from seven databases, including Asklepios (year 0 and year 10),⁷ Flemengho,⁸ CARDIA5 and CARDIA25,⁹ Padua 3D Echo Normal,¹⁰ and the Normal Reference Ranges for Echocardiography study,^{11,12} to obtain reference values in normal subjects for the left ventricle and the left atrium (see section 10). All data were obtained without the use of contrast agents. Data sets for all patients included age, gender, ethnicity, height, and weight. To ensure a normal population, subjects in these studies were excluded if any of the following criteria were met: systolic blood pressure > 140 mm Hg, diastolic blood pressure > 80 mm Hg, history of drug-treated hypertension, diagnosis of diabetes, impaired fasting glucose > 100 mg/dL, body mass index > 30 kg/m², creatinine > 1.3 mg/dL, estimated glomerular filtration rate < 60 mL/min/1.73 m², total cholesterol > 240 mg/dL, low-density lipoprotein cholesterol > 130 mg/dL, and total triglycerides > 150 mg/dL. Details of the statistical analysis are described in the Appendix. Because of varied study aims, not all echocardiographic measurements were available for each database. Supplemental Table 1 summarizes the sources of the data for each measurement group and their baseline characteristics.

Table 2 shows the normal values for 2D echocardiographic parameters of LV size and function according to gender, while Supplemental Table 2 provides expanded data for the same parameters, obtained from different echocardiographic views, and also includes the corresponding number of subjects used to obtain these data. Supplemental Table 3 lists normal ranges and consensus-based partition cutoffs for LV dimensions, volumes, EF, and mass. On multivariate analysis, age, gender, and BSA were found to have a significant independent influence on LV end-diastolic volume (EDV) and LV end-systolic volume (ESV). The results across genders and age deciles subdivided into absolute and BSA-normalized values are shown in Supplemental Table 4 (see Appendix).

Because ethnicity is an important factor, results of analysis by race and gender are presented in Supplemental Table 5. From the regression analysis, nomograms are provided for plotting observed LV dimensions versus BSA or BSA-indexed LV volumes versus age (Figures 1 and 2). Nomograms for absolute LV measurements against age (Supplemental Figures 1 and 2) and BSA (Supplemental Figures 3 and 4) are also provided (see Appendix).

1.4 Normal Reference Values for 3DE

Several studies have published 3D echocardiographic reference values for healthy normotensive subjects, which are summarized in Table 3.¹³ The reported variations in the normal ranges from study to study are likely due to differences in populations, echocardiographic equipment, and analysis software, as well as variability in measurement techniques. In patients with good image quality, the

accuracy of 3DE is comparable with that of CMR, although volumes tend to be lower on echocardiography.⁶

The effects of ethnicity on 3D echocardiographic LV volumes were investigated in one study, which reported that LV volumes were smaller among Asian Indians than white Europeans, but EF did not differ among ethnic groups.¹⁴ In most 3D echocardiographic studies, the relationship between age and 3D echocardiographic LV volumes was examined, and weak to moderate negative correlations were seen between age and LV volumes, while EF did not change significantly with age.^{10,15,16} This finding is similar to those described in the CMR literature.^{17,18} On the basis of weighted averages of three studies,^{16,19,20} 3D echocardiographic LV volumes were larger than 2D echocardiographic values, and corresponding upper limits of the normal range were EDVs of 79 mL/m² for men and 71 mL/m² for women and ESVs of 32 mL/m² for men and 28 mL/m² for women. Ultimately, a large study in a diverse population will be needed to establish normal reference ranges for 3DE for different ethnic groups.

Recommendation

LV size should be routinely assessed on 2DE by calculating volumes using the biplane method of disks summation technique. In laboratories with experience in 3DE, 3D measurement and reporting of LV volumes is recommended when feasible depending on image quality. When reporting LV linear dimensions, the recommended method is 2D-guided measurements. LV size and volume measurements should be reported indexed to BSA. For general reference, 2D echocardiographic LV EDVs of 74 mL/m² for men and 61 mL/m² for women and LV ESVs of 31 mL/m² for men and 24 mL/m² for women should be used as the upper limits of the corresponding normal range.

2. LV Global Systolic Function

Global LV function is usually assessed by measuring the difference between the end-diastolic and end-systolic value of a one-dimensional, 2D, or 3D parameter divided by its end-diastolic value. For this, end-diastole is preferably defined as the first frame after mitral valve closure or the frame in the cardiac cycle in which the respective LV dimension or volume measurement is the largest. End-systole is best defined as the frame after aortic valve closure or the frame in which the cardiac dimension or volume is smallest. In patients with regular heart rhythm, measurements of the timing of valve openings and closures derived from M-mode echocardiography, pulsed-wave (PW) or continuous-wave Doppler may be used for accurate definitions of ventricular time intervals.

2.1 Fractional Shortening

Fractional shortening can be derived from 2D-guided M-mode imaging or preferably from linear measurements obtained from 2D images. Deriving global LV function parameters from linear measurements is problematic when there are regional wall motion abnormalities due to coronary disease or conduction abnormalities. In patients with uncomplicated hypertension, obesity or valvular diseases, such regional differences are rare in the absence of clinically recognized myocardial infarction, and accordingly, this parameter may provide useful information in clinical studies.²¹ In patients with normal size of the LV base but enlarged midventricular and distal portions, LV

Table 2 Normal values for 2D echocardiographic parameters of LV size and function according to gender

Parameter	Male		Female	
	Mean \pm SD	2-SD range	Mean \pm SD	2-SD range
LV internal dimension				
Diastolic dimension (mm)	50.2 \pm 4.1	42.0–58.4	45.0 \pm 3.6	37.8–52.2
Systolic dimension (mm)	32.4 \pm 3.7	25.0–39.8	28.2 \pm 3.3	21.6–34.8
LV volumes (biplane)				
LV EDV (mL)	106 \pm 22	62–150	76 \pm 15	46–106
LV ESV (mL)	41 \pm 10	21–61	28 \pm 7	14–42
LV volumes normalized by BSA				
LV EDV (mL/m ²)	54 \pm 10	34–74	45 \pm 8	29–61
LV ESV (mL/m ²)	21 \pm 5	11–31	16 \pm 4	8–24
LV EF (biplane)	62 \pm 5	52–72	64 \pm 5	54–74

BSA, body surface area; EDV, end-diastolic volume; EF, ejection fraction; ESV, end-systolic volume; LV, left ventricular; SD, standard deviation.

volume would be a better marker of LV size than linear dimension measured at the LV base.

2.2 EF

EF is calculated from EDV and ESV estimates, using the following formula:

$$EF = (EDV - ESV)/EDV.$$

LV volume estimates may be derived from 2DE or 3DE, as described above (section 1.2). The biplane method of disks (modified Simpson's rule) is the currently recommended 2D method to assess LV EF by consensus of this committee. Table 4 lists 2DE-derived biplane LV EF, including normal ranges and consensus-based severity partition cutoffs according to gender. In patients with good image quality, 3DE-based EF measurements are accurate and reproducible and should be used when available and feasible.^{6,10,15,16,19,20}

2.3 Global Longitudinal Strain (GLS)

Lagrangian strain is defined as the change in length of an object within a certain direction relative to its baseline length:

$$\text{Strain}(\%) = (L_t - L_0)/L_0,$$

where L_t is the length at time t , and L_0 is the initial length at time 0. The most commonly used strain-based measure of LV global systolic function is GLS. It is usually assessed by speckle-tracking echocardiography (STE)^{22–24} (Table 1). On 2DE, peak GLS describes the relative length change of the LV myocardium between end-diastole and end-systole:

$$GLS(\%) = (MLs - MLd)/MLd,$$

where ML is myocardial length at end-systole (MLs) and end-diastole (MLd). Because MLs is smaller than MLd , peak GLS is a negative number. This negative nature of GLS can lead to confusion when describing increases or decreases in strain. We recommend that all references to strain changes specifically mention an increase or decrease in the absolute value of strain, to avoid confusion.

After optimizing image quality, maximizing frame rate, and minimizing foreshortening, which are all critical to reduce measurement variability, GLS measurements should be made in the three standard apical views and averaged.²⁵ Measurements should begin with the apical long-axis view to visualize aortic valve closure, using opening and closing clicks of the aortic valve or aortic valve opening and closing on M-mode imaging. When regional tracking is suboptimal in more than two myocardial segments in a single view, the calculation of GLS should be avoided. In such cases, alternative indices may be used to gain insight into longitudinal LV function, such as mitral annular plane systolic excursion or pulsed Doppler tissue imaging (DTI)-derived mitral annular peak systolic velocity (s').

There are concurrent definitions as a basis for GLS calculation using endocardial, midwall, or average deformation.²⁴ This committee refrains from recommendations in this regard and refers to the ongoing joint standardization initiative of the ASE, EACVI, and the ultrasound imaging industry.^{24,26} Because of intervendor and inter-software variability and age and load dependency, serial assessment of GLS in individual patients should be performed using the same vendor's equipment and the same software.

The preponderance of currently available data is for midwall GLS. Although the evidence base for its use in routine clinical echocardiography is far smaller than that for EF, measures of midwall GLS have been shown in several studies to be robust and reproducible²⁷ and to offer incremental predictive value in unselected patients undergoing echocardiography for the assessment of resting function,^{28,29} as well as in predicting postoperative LV function in patients with valve disease.^{30,31}

2.4 Normal Reference Values

Normal reference values for LV EF derived from 2DE have been updated using the population-based studies described in section 1.3 above. Details can be found in Tables 2 and 4 and Supplemental Tables 2–5 (see Appendix). EF is not significantly related to gender, age, or body size, as measured by BSA. Normal EF was $63 \pm 5\%$ using the biplane method of disks. Therefore, in individuals aged >20 years, EF in the range of 53% to 73% should be classified

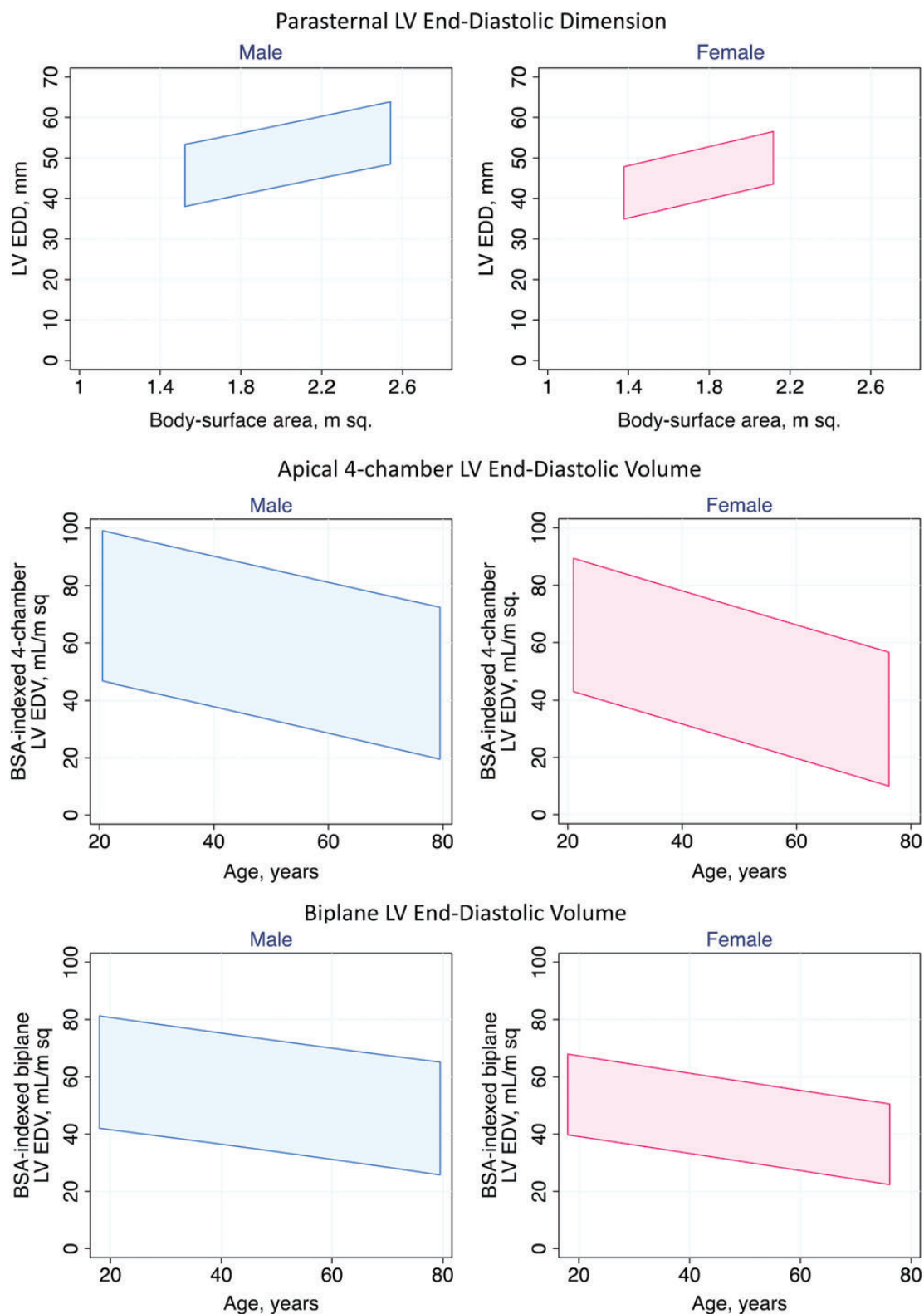


Figure 1 For men (left) and women (right), the 95% confidence intervals for the following measurements are presented: LV end-diastolic dimension measured from a parasternal long-axis window on the basis of BSA (top), BSA-indexed LV EDV measured from an apical four-chamber view on the basis of age (middle), and BSA-indexed biplane LV EDV on the basis of age (bottom). For example, a normal BSA-indexed LV EDV measured from the four-chamber view in a 40-year-old woman would fall between approximately 30 and 78 mL/m².

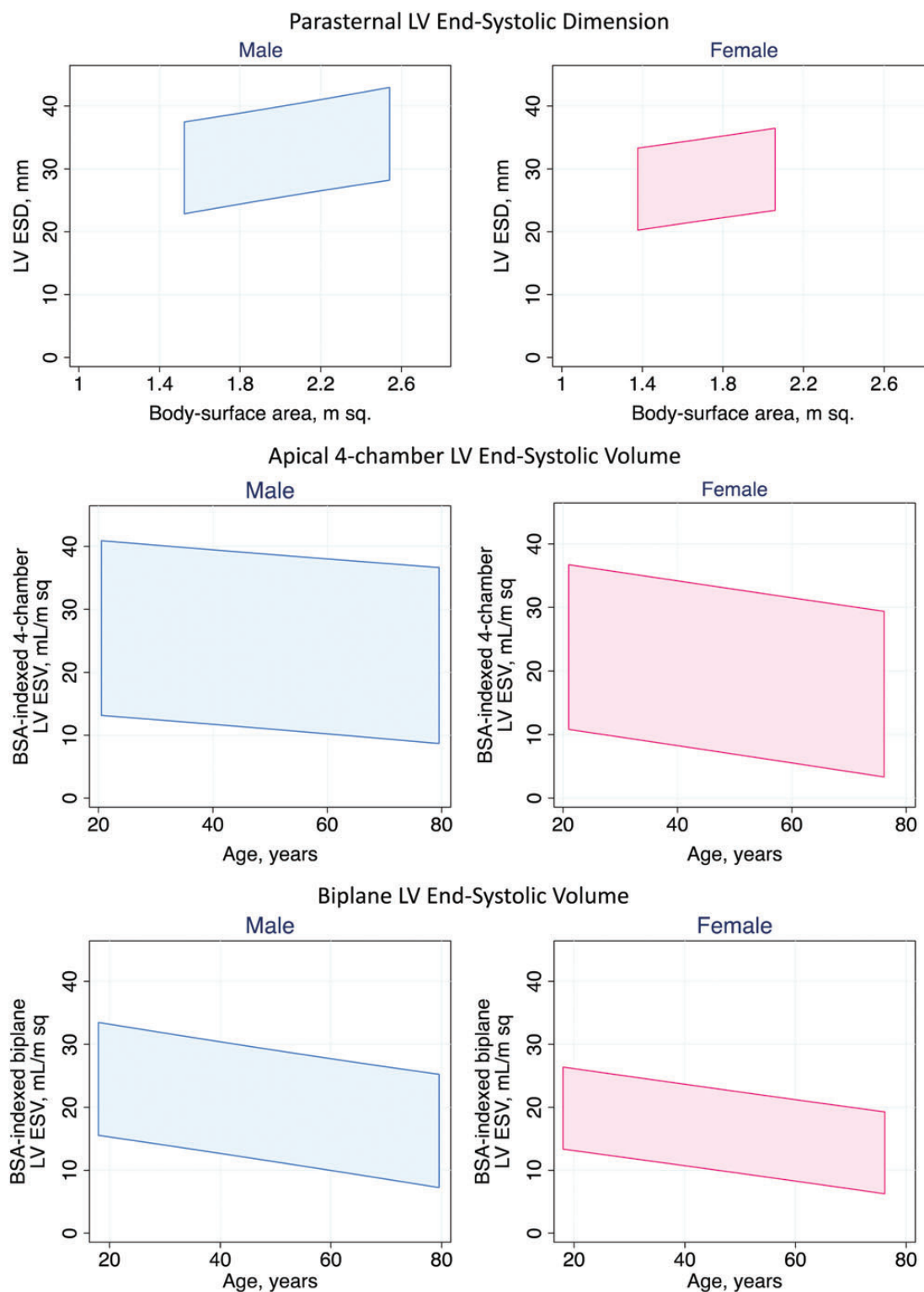


Figure 2 For men (left) and women (right), the 95% confidence intervals for the following measurements are presented: LV end-systolic dimensions measured from a parasternal long-axis window on the basis of BSA (top), BSA-indexed LV ESVs measured from an apical four-chamber view on the basis of age (middle), and BSA-indexed biplane LV ESVs based on age (bottom).

Table 3 Normal values for LV parameters obtained with 3DE

	Aune et al. (2010)	Fukuda et al. (2012)	Chahal et al. (2012)	Muraru et al. (2013)
Number of subjects	166	410	978	226
Ethnic makeup of population	Scandinavian	Japanese	51% European white, 49% Asian Indian	White European
EDVi (mL/m ²)				
Men, mean (LLN, ULN)	66 (46, 86)	50 (26, 74)	White: 49 (31, 67); Indian: 41 (23, 59)	63 (41, 85)
Women, mean (LLN, ULN)	58 (42, 74)	46 (28, 64)	White: 42 (26, 58); Indian: 39 (23, 55)	56 (40, 78)
ESVi (mL/m ²)				
Men, mean (LLN, ULN)	29 (17, 41)	19 (9, 29)	White: 19 (9, 29); Indian: 16 (6, 26)	24 (14, 34)
Women, mean (LLN, ULN)	23 (13, 33)	17 (9, 25)	White: 16 (8, 24); Indian: 15 (7, 23)	20 (12, 28)
EF (%)				
Men, mean (LLN, ULN)	57 (49, 65)	61 (53, 69)	White: 61 (49, 73); Indian: 62 (52, 72)	62 (54, 70)
Women, mean (LLN, ULN)	61 (49, 73)	63 (55, 71)	White: 62 (52, 72); Indian: 62 (52, 72)	65 (57, 73)

EDVi, LV EDV index; ESVi, LV ESV index; LLN, lower limit of normal; NR, not reported; RT3DTTE, real-time 3D TTE; SVi, LV stroke volume index; ULN, upper limit of normal. Modified with permission from Bhawe et al.¹³ LLN and ULN are defined as mean \pm 2 SDs.

Table 4 Normal ranges and severity partition cutoff values for 2DE-derived LV EF and LA volume

	Male				Female			
	Normal range	Mildly abnormal	Moderately abnormal	Severely abnormal	Normal range	Mildly abnormal	Moderately abnormal	Severely abnormal
LV EF (%)	52–72	41–51	30–40	<30	54–74	41–53	30–40	<30
Maximum LA volume/BSA (mL/m ²)	16–34	35–41	42–48	>48	16–34	35–41	42–48	>48

as normal. Three-dimensional echocardiographic normal values have been recently reported in different ethnic populations (Table 3).

Normal values for GLS depend on the definition of the measurement position in the myocardium, the vendor, and the version of the analysis software, resulting in considerable heterogeneity in the published literature.^{27,32,33} It is the consensus of this writing committee that differences among vendors and software packages are still too large to recommend universal normal values and lower limits of normal. To provide some guidance, a peak GLS in the range of –20% can be expected in a healthy person. A selection of recently published data is provided in the Appendix together with the lower normal limits (Supplemental Table 6). There is evidence that women have slightly higher absolute values of GLS than men and that strain values decrease with age.^{32,34} GLS is a valuable and sensitive tool for follow-up examinations, provided the same equipment, tracing methodology, and software are used.

Recommendations

LV systolic function should be routinely assessed using 2DE or 3DE by calculating EF from EDV and ESV. LV EFs of <52% for men and <54% for women are suggestive of abnormal LV systolic function. Two-dimensional STE-derived GLS appears to be reproducible and feasible for clinical use and offers incremental prognostic data over LV EF in a variety of cardiac conditions, although measurements vary among vendors and software versions. To provide some

guidance, a peak GLS in the range of –20% can be expected in a healthy person, and the lower the absolute value of strain is below this value, the more likely it is to be abnormal.

3. LV Regional Function

3.1 Segmentation of the Left Ventricle

For the assessment of regional LV function, the ventricle is divided into segments. Segmentation schemes should reflect coronary perfusion territories, result in segments with comparable myocardial mass, and allow standardized communication within echocardiography and with other imaging modalities (Figure 3). Accordingly, a 17-segment model is commonly used. Beginning at the anterior junction of the interventricular septum and the RV free wall and continuing counterclockwise, basal and midventricular segments should be labeled as anteroseptal, inferoseptal, inferior, inferolateral, anterolateral, and anterior. In this 17-segment model, the apex is divided into five segments, including septal, inferior, lateral, and anterior segments, as well as the “apical cap,” which is defined as the myocardium beyond the end of the LV cavity (Figures 3 and 4).³⁵ The 17-segment model may be used for myocardial perfusion studies or when comparing between different imaging modalities, specifically single photon-emission computed tomography, positron emission tomography, and CMR. Figure 5 shows a schematic representation of the perfusion territories of the three major coronary arteries. When using this

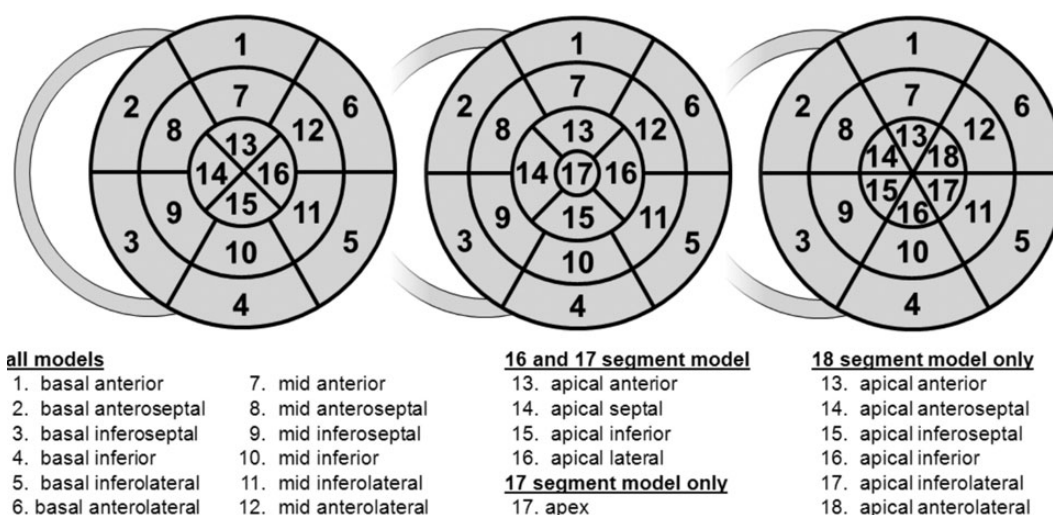


Figure 3 Schematic diagram of the different LV segmentation models: 16-segment model (left),³⁶ 17-segment model (center),³⁵ and 18-segment model (right). In all diagrams, the outer ring represents the basal segments, the middle ring represents the segments at midpapillary muscle level, and the inner ring represents the distal level. The anterior insertion of the right ventricular wall into the left ventricle defines the border between the anteroseptal and anterior segments. Starting from this point, the myocardium is subdivided into six equal segments of 60°. The apical myocardium in the 16- and 17-segment models is divided instead into four equal segments of 90°. In the 17-segment model an additional segment (*apical cap*) is added in the center of the bull's-eye. (modified from Voigt et al.²⁴).

17-segment model to assess wall motion or regional strain, the 17th segment (the apical cap) should not be included.

Alternative segmentation models treat the apex differently: the 16-segment model³⁶ divides the entire apex into the same four segments (septal, inferior, lateral, and anterior; Figure 3, left). Also, some segmentation schemes divide the apex into six segments, similar to the basal and midventricular levels, resulting in an 18-segment model (Figure 3, right) that is simple but results in a slight overrepresentation of the distal myocardium when scoring.

All segments can be visualized by 2DE. On average, the two-chamber view and the apical long-axis view intersect with the four-chamber view at angles of approximately 53° and 129°, respectively,³⁷ allowing the assessment of the central region of all segments from an apical window, independent of the model used. Although certain variability exists in the coronary artery blood supply to myocardial segments, segments are usually attributed to the three major coronary arteries (Figure 5).³⁵

3.2 Visual Assessment

In echocardiography, regional myocardial function is assessed on the basis of the observed wall thickening and endocardial motion of the myocardial segment. Because myocardial motion may be caused by adjacent segment tethering or overall LV displacement, regional deformation (thickening, shortening) should be the focus of the analysis. However, it must be recognized that deformation can also be passive and therefore may not always accurately reflect myocardial contraction.

It is recommended that each segment be analyzed individually in multiple views. A semiquantitative wall motion score can be assigned to each segment to calculate the LV wall motion score index as the

average of the scores of all segments visualized. The following scoring system is recommended: (1) normal or hyperkinetic, (2) hypokinetic (reduced thickening), (3) akinetic (absent or negligible thickening, e.g., scar), and (4) dyskinetic (systolic thinning or stretching, e.g., aneurysm).

An aneurysm is a morphologic entity that demonstrates focal dilatation and thinning (remodeling) with either akinetic or dyskinetic systolic deformation.³⁸ In contrast to the recommendation of previous guidelines,^{1,2} this committee refrains from assigning a separate wall motion score for aneurysm.

3.3 Regional Wall Motion during Infarction and Ischemia

Depending on the regional coronary flow reserve, stress echocardiography may reveal significant coronary artery stenoses by means of inducing a wall motion abnormality. Myocardial scar may also result in regional dysfunction of variable severity. Echocardiography can over- or underestimate the amount of ischemic or infarcted myocardium, depending on the function of adjacent regions, regional loading conditions, and stunning.³⁹ In stress echocardiography, visual recognition of regional dysfunction can be improved with a synchronized side-by-side comparison of baseline and stress images using digital technology.⁴⁰

3.4 Regional Abnormalities in the Absence of Coronary Artery Disease

Regional wall motion abnormalities may also occur in the absence of coronary artery disease, in a variety of conditions, such as myocarditis, sarcoidosis, and stress-induced (takotsubo) cardiomyopathy. Abnormal motion patterns of the interventricular septum may be found postoperatively or in the presence of a left bundle branch block or RV

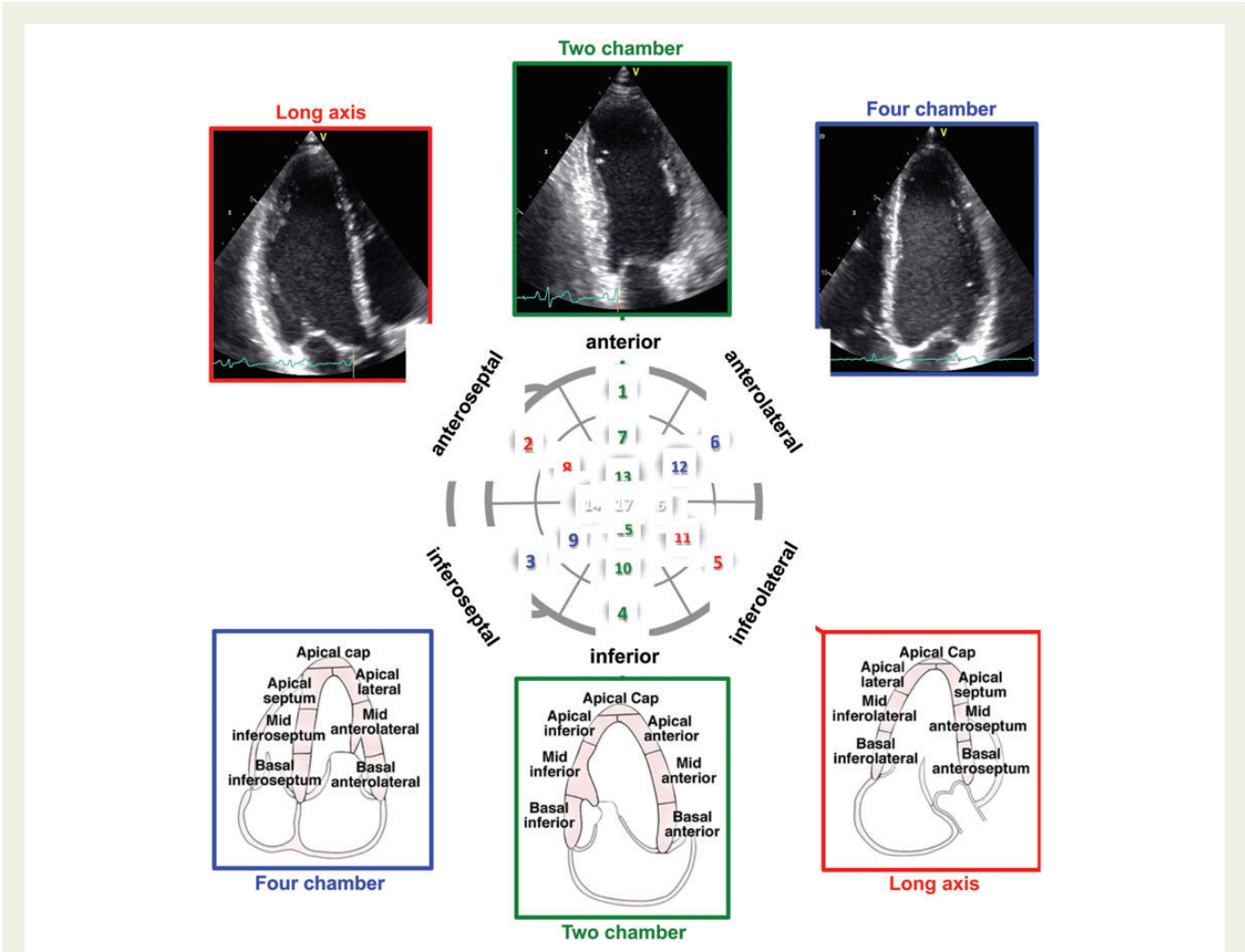


Figure 4 Orientation of apical four-chamber (A4C), apical two-chamber (A2C), and apical long-axis (ALX) views in relation to the bull's-eye display of the LV segments (center). Top panels show actual images, and bottom panels schematically depict the LV wall segments in each view.

epicardial pacing, as well as RV dysfunction caused by RV pressure or volume overload. Furthermore, some conduction delays can cause regional wall motion abnormalities in the absence of primary myocardial dysfunction. This regional dysfunction is due to the abnormal sequence of myocardial activation, which causes heterogeneous loading conditions and remodeling.⁴¹ Ideally, the temporal sequence of activation and motion should be described. Characteristic motion patterns, which result from abnormal activation sequences, such as septal bounce (“beaking,” “flash”) or lateral apical motion during systole (“apical rocking”) should be reported.^{42–45}

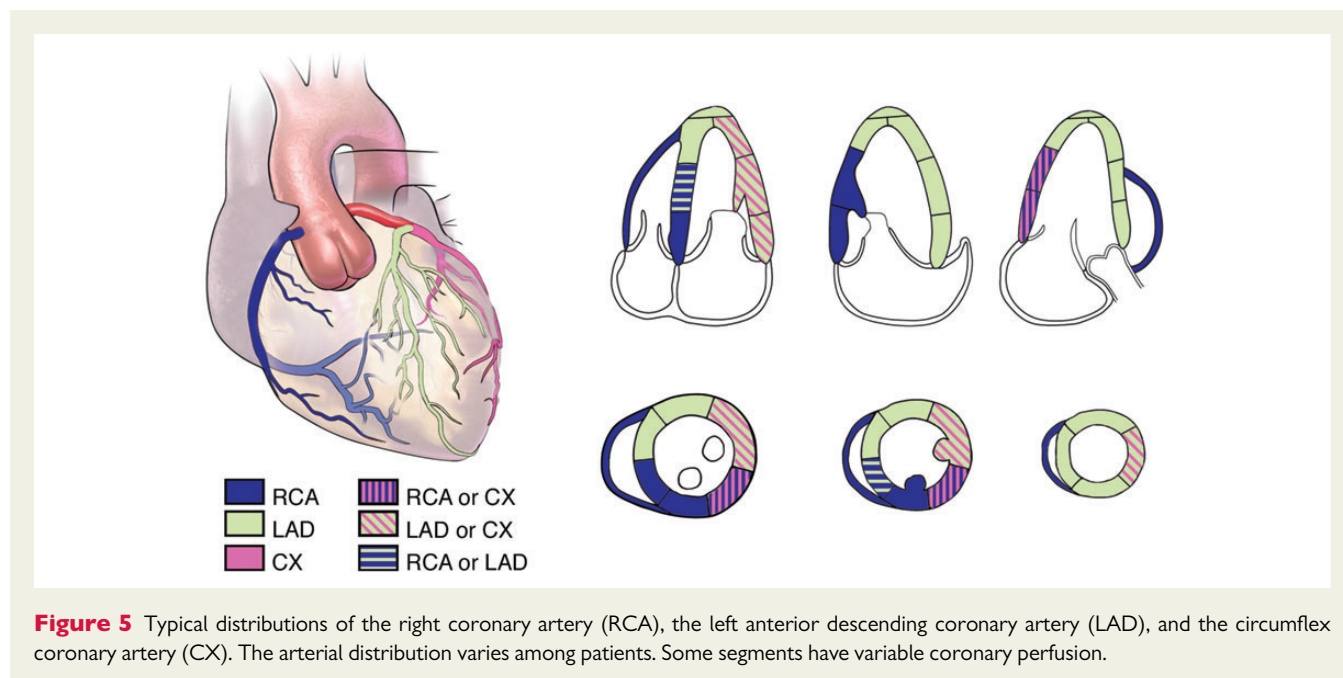
3.5 Quantification of Regional Wall Motion Using Doppler and STE

Echocardiographic quantification of regional myocardial function is currently based on DTI or speckle-tracking echocardiographic techniques.^{46–48} Both techniques provide comparable data quality, although DTI is known to be angle dependent and prone to underestimating motion that is not parallel to the ultrasound beam. Commonly used parameters include velocity, motion, deformation, and

deformation rate. Because velocity and motion are measured relative to the transducer, measurements may be influenced by tethering or overall heart motion. Accordingly, the use of deformation parameters, such as strain and strain rate, is preferable.

The most commonly used deformation parameter is longitudinal strain during LV systole. Similar to global strain, with current technology, regional deformation measurements may vary in amplitude, depending on the myocardial region being investigated, the measurement methodology, the vendor, and sample volume definition. Therefore, no specific normal ranges are provided in this document. These values await the upcoming consensus document of the joint task force of the ASE, EACVI, and the industry for the standardization of quantitative function imaging.^{23,25}

Independent of strain magnitude, characteristic changes in temporal pattern of myocardial deformation can be assessed as well. Longitudinal shortening or radial thickening of the myocardium after aortic valve closure (postsystolic shortening or thickening, sometimes referred to as tardokinesis) of > 20% of the total deformation during the cardiac cycle is a consistent sign of regional functional



inhomogeneity (e.g., ischemia, scar).⁴⁴ The development of postsystolic shortening during a stress test has been proposed as an indicator of regional ischemia.⁴⁹ The value of regional deformation parameters and temporal patterns of strain derived by speckle-tracking from either 2D or 3D echocardiographic data sets is the subject of ongoing research and remains to be determined.^{50,51}

Recommendations

Different LV segmentation models are used in clinical practice. The 17-segment model is recommended to assess myocardial perfusion with echocardiography and other imaging techniques. The 16-segment model is recommended for routine studies assessing wall motion, because endocardial excursion and thickening of the tip of the apex are imperceptible. To assess wall motion, each segment should be evaluated in multiple views and a four-grade scoring should be applied: (1) normal or hyperkinetic, (2) hypokinetic (reduced thickening), (3) akinetic (absent or negligible thickening), and (4) dyskinetic (systolic thinning or stretching). Despite promising data, quantitative assessment of the magnitude of regional LV deformation cannot be recommended at this stage because of lack of reference values, suboptimal reproducibility, and considerable inter-vendor measurement variability.

4. LV Mass

LV mass is an important risk factor for, and a strong predictor of, cardiovascular events.^{52–55} There are several methods that effectively calculate LV mass from M-mode echocardiography, 2DE, and 3DE (Table 5). All measurements should be performed at the end of diastole (the frame before mitral valve closure or the frame in the cardiac cycle in which the ventricular dimension or volume is largest). Those that use M-mode (either blinded or 2D-guided) and 2D echocardiographic linear measurements of LV diastolic diameter and wall thickness rely on geometric formulas to calculate the volume

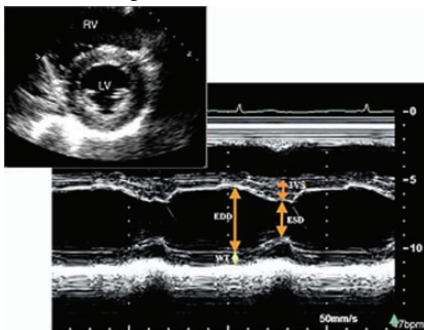
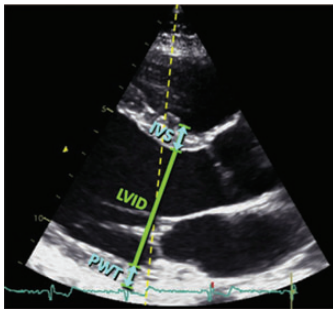
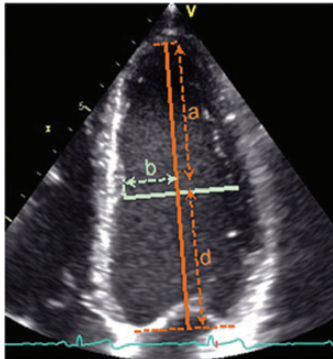
of LV myocardium, while 3DE can measure it directly. All methods then convert the volume to mass by multiplying the volume of myocardium by the myocardial density (approximately 1.05 g/mL).

When the entire ventricle is measured from 2D echocardiographic images, either the area-length or truncated ellipsoid technique is used.¹ Each method for LV mass measurement has advantages, disadvantages, and value in specific situations (Table 5).

To measure LV mass in an individual patient over time, especially those with cardiac disease, the 2D echocardiographic methods have advantages compared with the linear dimension technique.¹ There are, however, fewer studies of the prognostic value of LV mass calculated by these methods compared with the linear dimension method described below. Unlike the linear dimension or M-mode method, the 2D echocardiographic methods can accommodate for the shape of the ventricle and account for changes in LV size that might occur along the long axis of the chamber. This is an important consideration, because changes in LV geometry are common in various cardiac diseases.

However, when there is a need to screen or study large populations, the M-mode method has advantages, because it is simple, quick, and subject to less measurement variability. There is a large body of evidence to support the accuracy of this method. Most studies that relate LV mass to prognosis are based on this method.⁵⁶ However, several caveats need to be mentioned. First, it is critical that the wall thickness and LV dimensions measured be truly perpendicular to the long axis of the left ventricle. Therefore, 2D-guided M-mode imaging or measurements from 2D echocardiographic images are preferred over blind M-mode imaging. Second, the formula includes a correction for the 20% overestimation that was found during the original validation studies of the M-mode technique. Because direct 2D measures of wall thickness may yield smaller values than the M-mode technique, LV mass calculated using this formula may not be directly interchangeable (Table 5). This may be

Table 5 Recommendations for the echocardiographic assessment of LV mass

Parameter and method	Echocardiographic imaging	Advantages	Limitations
Linear method Cube formula $\text{LV mass} = 0.8 \cdot 1.04 \cdot [(\text{IVS} + \text{LVID} + \text{PWT})^3 - \text{LVID}^3] + 0.6 \text{ g}$ <p>Where IVS is interventricular septum; LVID is LV internal diameter, and PWT is inferolateral wall thickness.</p> <p>Linear internal measurements of the LV should be acquired from the parasternal approach and carefully obtained perpendicular to the LV long axis, and measured at the level of the mitral valve leaflet tips. M-mode measurements should be obtained from a targeted SAX or a parasternal LAX view. All measurements should be performed at end-diastole.</p>	M-mode tracing 	<ul style="list-style-type: none"> Fast and widely used Wealth of published data Demonstrated prognostic value Fairly accurate in normally shaped ventricles (i.e., systemic hypertension, aortic stenosis) Simple for screening large populations 	<ul style="list-style-type: none"> Based on the assumption that the left ventricle is a prolate ellipsoid with a 2:1 long/short axis ratio and symmetric distribution of hypertrophy Beam orientation frequently off axis Since linear measurements are cubed, even small measurement errors in dimensions or thickness have an impact on accuracy Overestimates LV mass Inaccurate in the presence of asymmetric hypertrophy, dilated ventricles and other diseases with regional variations in wall thickness
2D based formulas Truncated ellipsoid: $\text{LV mass} = 1.05\pi \left\{ (b+t)^2 \left[\frac{2}{3}(a+t) + d - \frac{d^3}{3(a+t)^2} \right] - b^2 \left[\frac{2}{3}a + d - \frac{d^3}{3a^2} \right] \right\}$	2D 	<ul style="list-style-type: none"> Facilitates orientation perpendicular to the LV long axis Partial correction for shape distortions Less dependent on geometrical assumptions than the linear measurements 	<ul style="list-style-type: none"> Based on the same geometrical assumptions as M-mode Same limitations as M-mode in patients with abnormal LV geometry Impact of harmonic imaging on the mass calculations and normal values remains to be defined Normal values are less well established than for M-mode measurements
		<ul style="list-style-type: none"> Good image quality and properly oriented parasternal short-axis views (no oblique planes) are required Good epicardial definition is required Cumbersome methodology Higher measurement variability Few published normative data Limited prognostic data 	

Area-length:

$$\text{LV mass} = 1.05$$

$$\left\{ \left[\frac{5}{6} A_1 (a + d + t) \right] - \left[\frac{5}{6} A_2 (a + d) \right] \right\}$$

Mean wall thickness is calculated from epicardial (A_1) and endocardial (A_2) cross-sectional areas in short-axis view at the papillary muscle level (top panel, green line) with the papillary muscles considered part of the LV cavity. The short axis radius is calculated as:

$$b \sqrt{\frac{A_2}{\pi}}$$

Then, mean wall thickness t is calculated as:

$$t = \left(\sqrt{\frac{A_1}{\pi}} \right) - b$$

and the cross sectional area of the myocardium (A_m) in short-axis view is:

$$A_m = A_1 - A_2$$

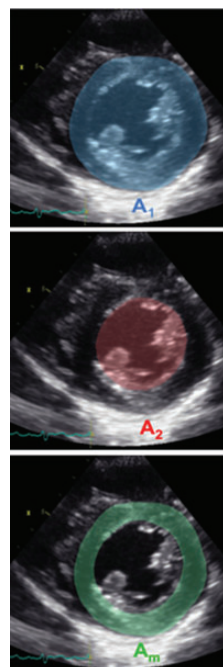
LV mass is calculated from these measurements plus the LV length measured from the level of the short axis plane to the base (d) and to the apex (a).

Key: a - distance from the minor axis to the endocardium at the LV apex; b = LV minor radius; d - distance from the minor axis to the mitral valve plane; t - mean wall thickness.

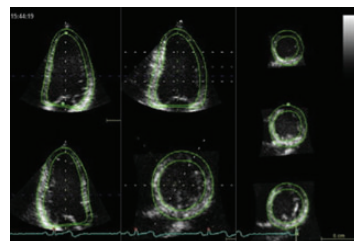
LV mass = (LV epicardial volume - LV endocardial volume). 1.05 = LV myocardial volume. 1.05

LV mass = (LV epicardial volume - LV endocardial volume). 1.05 = LV myocardial volume. 1.05

3D based formula



3D data set



- Direct measurement without geometrical assumptions about cavity shape and hypertrophy distribution
- More accurate than the linear or the 2D measurements
- Higher inter-measurement and test/re-test reproducibility
- Better discriminates small changes within a patient
- Normal values less well established
- Dependent on image quality
- Patient's cooperation required

a less important consideration if the method is being used to identify cutoff values for prognosis. It is also important to note that the formula raises the linear dimensions to the power of 3, and thus even small errors in dimensions can have significant effects on the calculated LV mass.

Most studies that have compared 2D-guided M-mode measurements of LV mass with the 2D echocardiographic area-length or truncated ellipsoid methods in normally shaped ventricles have shown subtle differences but no clear advantage of one technique over the other.⁵⁷ However, comparison studies have not been performed in the current era, when tremendous gains in 2D echocardiographic image quality have been made. In fact, large population studies confirming or reestablishing normal values for LV mass with harmonic imaging are limited.^{58,59}

Because 3DE is the only echocardiographic method that directly measures myocardial volume, it is an appropriate approach. Numerous validation studies have been performed.⁶⁰ However, to date, there have been few studies assessing its practical use, feasibility, variability, or prognostic value in large-scale clinical environments.⁶¹ Accordingly, it is the consensus of this committee that the 3D echocardiographic LV mass data available in normal subjects are not sufficient to recommend normal reference values. It must also be noted that continuous improvements in the spatial and temporal resolution of 3D echocardiographic imaging will also influence normal values and measurement variability.

In patients with upper septal hypertrophy, the linear dimension methods, which use basal ventricular measurements, result in overestimation of the true mass, because the thickest region of the interventricular septum is incorporated in the measurement. In contrast, the area-length method, which uses mid-ventricular measurements, underestimates LV mass, because the thickest part of the interventricular septum is not included in the measurement. In the setting of discrete upper septal or asymmetric hypertrophy, if these methods are used to serially assess LV mass in a patient, it is critical to use the same methodology over time and to measure the walls at the same level of the ventricle. The 3D method has the advantage of accommodating regional differences in wall thickness and therefore can provide the most accurate measurements of LV mass in this setting.

The values for LV mass vary according to gender, age, body size, obesity, and region of the world. Therefore, uniform reference values are difficult to define. LV mass is higher in men independent of body size and increases with body size. Since the publication of the 2005 recommendations, several studies, mostly using linear measurements, have reported normal values of LV mass in normal populations.^{59,62–66} The larger studies reported values close to those recommended in the previous guidelines.^{62,65,66} Therefore, the same reference values and abnormality partition cutoffs as reported in the previous guidelines continue to be recommended (Table 6). However, characterization of the population being studied, and differences in mass between different ethnic populations should be taken into account when determining normal values.^{10,16,67–69}

The indexing of LV mass allows comparisons in subjects with different body sizes. However, whether to use height, weight, or BSA as the indexing term remains controversial. Studies suggest that indexing to height raised to allometric powers such as 1.7, 2.13, and 2.7 has advantages over indexing to BSA, especially when attempting to

Table 6 Normal ranges for LV mass indices

	Women	Men
Linear method		
LV mass (g)	67–162	88–224
<i>LV mass/BSA (g/m²)</i>	<i>43–95</i>	<i>49–115</i>
Relative wall thickness (cm)	0.22–0.42	0.24–0.42
<i>Septal thickness (cm)</i>	<i>0.6–0.9</i>	<i>0.6–1.0</i>
<i>Posterior wall thickness (cm)</i>	<i>0.6–0.9</i>	<i>0.6–1.0</i>
2D method		
LV mass (g)	66–150	96–200
<i>LV mass/BSA (g/m²)</i>	<i>44–88</i>	<i>50–102</i>

Bold italic values: recommended and best validated.

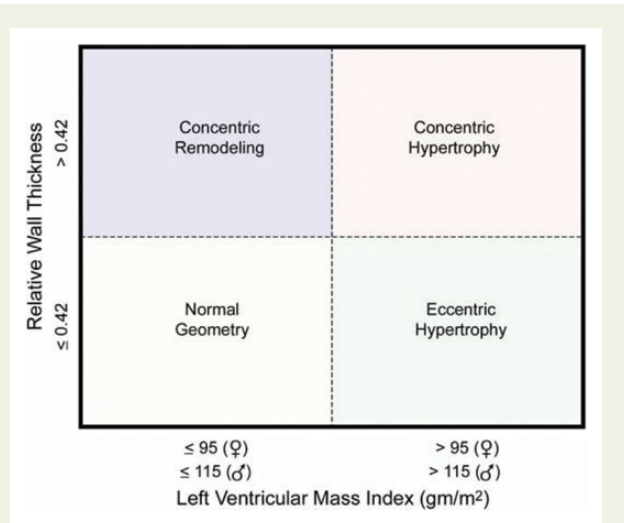


Figure 6 Comparison of RWT. Patients with normal LV mass can have either concentric remodeling (normal LV mass with increased RWT ≥ 0.42) or normal geometry (RWT ≤ 0.42) and normal LV mass. Patients with increased LV mass can have either concentric (RWT ≥ 0.42) or eccentric (RWT ≤ 0.42) hypertrophy. These LV mass measurements are based on linear measurements.

predict events in obese patients.^{65,70} However most large population studies reporting LV mass have indexed to BSA.

Finally, calculation of relative wall thickness (RWT) with the formula $(2 \times \text{posterior wall thickness})/(\text{LV internal diameter at end-diastole})$ permits categorization of an increase in LV mass as either concentric (RWT > 0.42) or eccentric (RWT ≤ 0.42) hypertrophy and allows the identification of concentric remodeling (normal LV mass with increased RWT) (Figure 6).

Recommendations

In the normally shaped left ventricle, both M-mode and 2D echocardiographic formulas to calculate LV mass can be used. Normal values for these techniques remain unchanged from the previous guidelines

and should be reported indexed to BSA. Reference upper limits of normal LV mass by linear measurements are 95 g/m² in women and 115 g/m² in men. Reference upper limits of normal LV mass by 2D measurements are 88 g/m² in women and 102 g/m² in men with 2D methods. Because 3DE is the only echocardiographic technique that measures myocardial volume directly, without geometric assumptions regarding LV shape and distribution of wall thickening, this technique is promising and may be used in abnormally shaped ventricles or in patients with asymmetric or localized hypertrophy. Limited upper normal limits of 3D echocardiographic LV mass data are currently available in the literature but are insufficient to substantiate recommendations for reference values.

II. The Right Ventricle

The right ventricle has a unique crescent shape, which adds complexity to the quantification of its size and function. This chamber plays an important role in the morbidity and mortality of patients presenting with signs and symptoms of cardiopulmonary disease. Until recently, little uniformity in echocardiographic imaging of the right heart existed because of a lack of familiarity with various techniques, and the enormous attention directed toward left heart quantification. The ASE has recently published a guidelines document, endorsed by the EACVI and the Canadian Society of Echocardiography, standardizing the approach for the evaluation of right heart dimensions and function during echocardiographic assessment of the right heart in adults.⁷¹ Compared with that document, this section provides updated reference values for RV dimensions and most parameters of systolic and diastolic function, which should replace the previously published guideline.

5. General Recommendations for RV Quantification

In all clinical studies, a comprehensive examination of the right ventricle should be performed, taking into account the study indication and available clinical information. The operator should examine the right ventricle using multiple acoustic windows, and the report should present an assessment based on both qualitative and quantitative parameters. Parameters that can be measured include RV and right atrial (RA) size, a measure of RV systolic function, as assessed by at least one or a combination of the following: fractional area change (FAC), DTI-derived tricuspid lateral annular systolic velocity wave (S'), tricuspid annular plane systolic excursion (TAPSE), and RV index of myocardial performance (RIMP). RV systolic pressure, typically calculated using the tricuspid regurgitation jet and an estimation of RA pressure based on inferior vena cava (IVC) size and collapsibility, should be reported when a complete TR Doppler velocity envelope is present.⁷¹ When feasible, additional parameters such as RV volumes and EF using 3DE should complement the basic 2D echocardiographic measurements listed above. The recommended methods, as well as the advantages and limitations of each parameter, are summarized in *Tables 7* and *9*, whereas the new reference values are displayed in *Tables 8* and *10*. These reference values are based on published mean and SD data obtained from normal adult individuals without any histories of heart or pulmonary disease (*Supplemental Table 7*). This document

uses the same methodology as in the previous RV guidelines, whereby a meta-analysis was performed for each parameter.

Not all of the recommended values are identical to those published in the previous guidelines.⁷¹ On the basis of the inclusion of new data published in recent reports, minor changes were made in the cutoff values for RV dimension, S', TAPSE, and RIMP. New publications since the last guidelines have resulted in changes in the reference values for 3DE-derived RV EF and volumes (*Tables 8* and *10*). It is important for the reader to recognize that most of the values proposed are not indexed to gender, BSA, or height, despite data suggesting the advantages of indexing.^{72–75} As a result, it is possible that patients at either extreme of height or BSA may be misclassified as having values outside the reference ranges, and it is recommended that the interpreting physician consider these parameters when generating the report. This potential misclassification also applies to other groups, such as patients with congenital heart disease and endurance athletes, for whom specific reference values are nonexistent.⁷⁶

6. Essential Imaging Windows and Views

Apical four-chamber, RV-focused apical four-chamber and modified apical four-chamber (*Figure 7A*), left parasternal long- and short-axis, left parasternal RV inflow, and subcostal views provide the images required for a comprehensive assessment of RV size, systolic and diastolic function, and RV systolic pressures.⁷¹ In most cases, in the RV-focused view, visualization of the entire RV free wall is better than in a standard four-chamber view, which is centered on the left ventricle. It is therefore recommended that to measure the right ventricle, a dedicated view focused on the right ventricle be used. *Figure 7A* and *Table 7* show the different RV views and recommendations for measurements.

7. RV Measurements

7.1 Linear Measurements

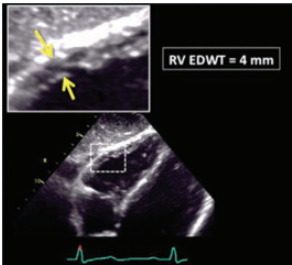
Quantitation of RV dimensions is critical and reduces interreader variability compared with visual assessment alone.⁷⁷ Measurements by 2DE are challenging because of the complex geometry of the right ventricle and the lack of specific right-sided anatomic landmarks to be used as reference points. The conventional apical four-chamber view (i.e., focused on the left ventricle) results in considerable variability in how the right heart is sectioned, and consequently, RV linear dimensions and areas may vary widely in the same patient with relatively minor rotations in transducer position (*Figure 7B*). RV dimensions are best estimated from a RV-focused apical four-chamber view obtained with either lateral or medial transducer orientation (*Figure 7A* and *Table 7*). Care should be taken to obtain the image with the LV apex at the center of the scanning sector, while displaying the largest basal RV diameter and thus avoiding foreshortening. Of note, the accuracy of RV measurements may be limited when the RV free wall is not well defined because of the dimension of the ventricle itself or its position behind the sternum. Recent data have suggested that indexing RV “size” to BSA may be relevant in some circumstances, but the measurements used in those studies lacked the reference points of the RV-focused view and frequently used RV areas, rather than linear dimensions.^{73,74} Reference values for RV dimensions are listed in *Table 8*. In general, a diameter <41 mm at the base and >35 mm at the midlevel in the RV-focused view indicates RV dilatation.

Table 7 Recommendations for the echocardiographic assessment of RV size

Echocardiographic imaging	Recommended methods	Advantages	Limitations
RV linear dimensions (inflow)* 	<ul style="list-style-type: none"> Basal RV linear dimension (RVD1) = maximal transversal dimension in the basal one third of RV inflow at end-diastole in the <i>RV-focused</i> view Mid-cavity RV linear dimension (RVD2) = transversal RV diameter in the middle third of RV inflow, approximately halfway between the maximal basal diameter and the apex, at the level of papillary muscles at end-diastole. 	<ul style="list-style-type: none"> Easily obtainable Simple Fast Wealth of published data 	<ul style="list-style-type: none"> RV size may be underestimated due to the crescent RV shape RV linear dimensions are dependent on probe rotation and different RV views; in order to permit inter-study comparison, the echocardiography report should state the window from which the measurement was performed.
RV linear dimensions (outflow)* 	<ul style="list-style-type: none"> Proximal RV outflow diameter (RVOT prox) = linear dimension measured from the anterior RV wall to the interventricular septal-aortic junction (in parasternal long-axis view) or to the aortic valve (in parasternal short-axis) at end-diastole Distal RV outflow diameter (RVOT distal) = linear transversal dimension measured just proximal to the pulmonary valve at end-diastole 	<ul style="list-style-type: none"> Easily obtainable Simple Fast 	<ul style="list-style-type: none"> RVOT prox is dependent on imaging plane position and less reproducible than RVOT distal Risk of underestimation or overestimation if the RV view is obliquely oriented with respect to RV outflow tract RV outflow dimensions can be inaccurate in case of chest and spine deformities Endocardial definition of the RV anterior wall is often suboptimal Limited normative data is available Regional measure; may not reflect global RV size (underestimation or overestimation)
RV areas (inflow) 	<ul style="list-style-type: none"> Manual tracing of RV endocardial border from the lateral tricuspid annulus along the free wall to the apex and back to medial tricuspid annulus, along the interventricular septum at end-diastole and at end-systole Trabeculations, papillary muscles and moderator band are included in the cavity area 	<ul style="list-style-type: none"> Relatively easy to measure 	<ul style="list-style-type: none"> Challenging in case of suboptimal image quality of RV free wall Challenging in the presence of trabeculation RV size underestimation if RV cavity is foreshortened Due to the LV twisting motion and the crescent RV shape, the end-diastolic RV image may not be in the same tomographic plane as the end-systolic one May not accurately reflect global RV size (underestimation or overestimation)
3DE RV volumes 	<ul style="list-style-type: none"> Dedicated multibeam 3D acquisition, with minimal depth and sector angle (for a temporal resolution >20–25 volumes/sec) that encompasses entire RV cavity Automatically identified timing of end-diastole and end-systole should be verified Myocardial trabeculae and moderator band should be included in the cavity 	<ul style="list-style-type: none"> Unique measures of RV global size that includes inflow, outflow and apical regions Independent of geometric assumptions Validated against cardiac magnetic resonance 	<ul style="list-style-type: none"> Dependent on image quality, regular rhythm, patient cooperation Needs specific 3D echocardiographic equipment and training Reference values established in few publications

Continued

Table 7 Continued

Echocardiographic imaging	Recommended methods	Advantages	Limitations
RV wall thickness 	<ul style="list-style-type: none"> Linear measurement of RV free wall thickness (either by M-mode or 2DE) performed at end-diastole, below the tricuspid annulus at a distance approximating the length of anterior tricuspid leaflet, when it is fully open and parallel to the RV free wall. Trabeculae, papillary muscles and epicardial fat should be excluded Zoomed imaging with focus on the RV mid-wall and respiratory maneuvers may improve endocardial border definition 	<ul style="list-style-type: none"> Easy to perform 	<ul style="list-style-type: none"> Single-site measurement Harmonic imaging and oblique M-mode sampling may overestimate RV wall thickness Challenging in case of thickening of visceral pericardium There is no criterion for defining an abnormally thin RV wall

*All linear dimensions should be obtained using inner-edge-to-inner-edge method.

Table 8 Normal values for RV chamber size

Parameter	Mean \pm SD	Normal range
RV basal diameter (mm)	33 \pm 4	25–41
RV mid diameter (mm)	27 \pm 4	19–35
RV longitudinal diameter (mm)	71 \pm 6	59–83
RVOT PLAX diameter (mm)	25 \pm 2.5	20–30
RVOT proximal diameter (mm)	28 \pm 3.5	21–35
RVOT distal diameter (mm)	22 \pm 2.5	17–27
RV wall thickness (mm)	3 \pm 1	1–5
RVOT EDA (cm ²)		
Men	17 \pm 3.5	10–24
Women	14 \pm 3	8–20
RV EDA indexed to BSA (cm ² /m ²)		
Men	8.8 \pm 1.9	5–12.6
Women	8.0 \pm 1.75	4.5–11.5
RV ESA (cm ²)		
Men	9 \pm 3	3–15
Women	7 \pm 2	3–11
RV ESA indexed to BSA (cm ² /m ²)		
Men	4.7 \pm 1.35	2.0–7.4
Women	4.0 \pm 1.2	1.6–6.4
RV EDV indexed to BSA (mL/m ²)		
Men	61 \pm 13	35–87
Women	53 \pm 10.5	32–74
RV ESV indexed to BSA (mL/m ²)		
Men	27 \pm 8.5	10–44
Women	22 \pm 7	8–36

EDA, end-diastolic area; ESA, end-systolic area; PLAX, parasternal long-axis view; RVOT, RV outflow tract.

7.2 Volumetric Measurements

Three-dimensional echocardiography allows measurements of RV volumes (Figure 8), thereby overcoming the limitations of conventional 2DERV views with respect to orientation and reference points. Although technically challenging, particularly in patients with

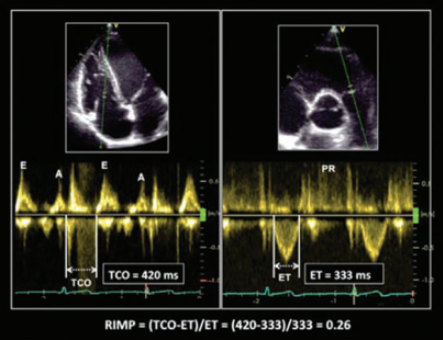
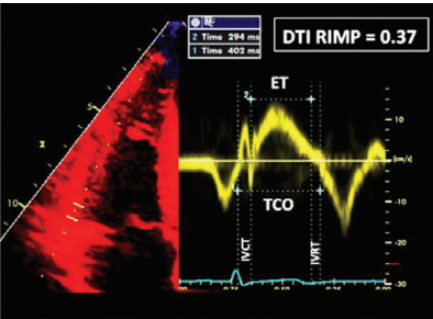
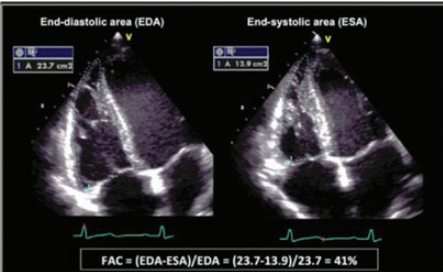
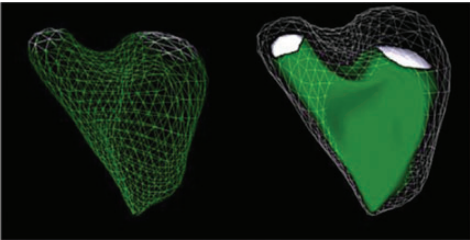
imperfect image quality or severely enlarged right ventricles, a reasonably accurate estimate of RV EDV and ESV can be obtained, and RV EF can be calculated.

Practical recommendations regarding RV 3D imaging and analysis have been recently published by the European Association of Echocardiography and the ASE.⁶¹ During analysis of RV volume, it is critically important to manually define end-diastolic and end-systolic frames using maximal and minimal RV volumes, respectively, rather than LV chamber changes (Table 7). Myocardial trabeculae and the moderator band should be included in the cavity, and RV contours on dynamic images should closely follow endocardial displacement and excursion of the tricuspid annulus throughout the cardiac cycle.

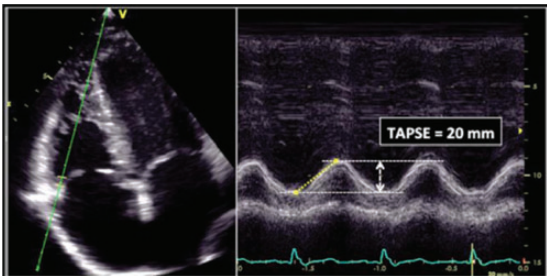
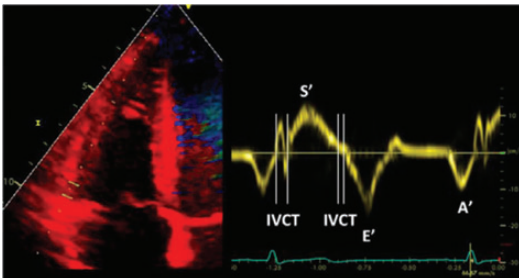
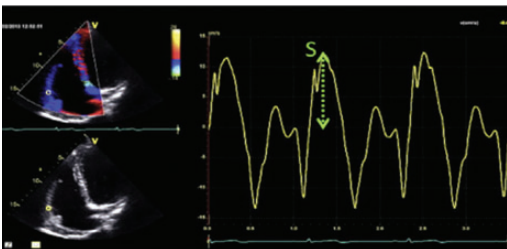
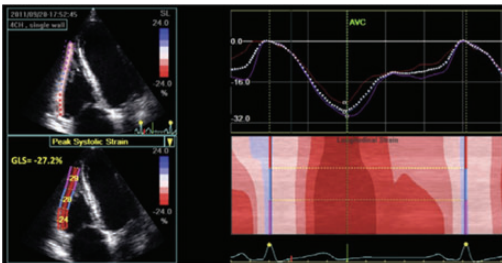
Even though 3DE tends to underestimate RV volumes compared CMR,⁷⁸ 3DE has identified relationships between RV volumes and EF to age and gender, which are very similar to those described by CMR.⁷² Overall, women have smaller 3D echocardiographic RV volumes, despite indexing to BSA, and higher EFs.⁷⁵ Also, older age is associated with smaller volumes (expected decrements of 5 mL/decade for EDV and 3 mL/decade for ESV) and higher EF (an expected increment of 1% per decade).⁷⁵ Reference values of 3DE-derived RV volumes (indexed to BSA) and EF obtained from the meta-analyses of all studies are summarized in Tables 8 and 10. Details of the above-described study factoring in age, gender, and BSA are listed in Supplemental Table 8.⁷⁵ Although RV volumes by CMR appear to be significantly influenced by race,⁷² no 3D echocardiographic data are yet available.

Recommendations

RV size should be routinely assessed by conventional 2DE using multiple acoustic windows, and the report should include both qualitative and quantitative parameters. In laboratories with experience in 3DE, when knowledge of RV volumes may be clinically important, 3D measurement of RV volumes is recommended. Although normal 3D echocardiographic values of RV volumes need to be established in larger groups of subjects, current published data suggest RV EDVs of 87 mL/m² in men and 74 mL/m² in women, and RV ESVs of 44 mL/m² for men and 36 mL/m² for women as the upper limits of the corresponding normal ranges.

Table 9 Recommendations for the echocardiographic assessment of RV function			
Echocardiographic imaging	Recommended methods	Advantages	Limitations
RV global function Pulsed Doppler RIMP	RIMP (Tei index) by pulsed Doppler: $RIMP = (TCO - ET)/ET$	<ul style="list-style-type: none">• Prognostic value• Less affected by heart rate	<ul style="list-style-type: none">• Requires matching for R-R intervals when measurements are performed on separate recordings• Unreliable when RA pressure is elevated
			
Tissue Doppler RIMP	RIMP by tissue Doppler: $RIMP = (IVRT + IVCT)/ET$ $ET = (TCO - ET)/ET$	<ul style="list-style-type: none">• Less affected by heart rate• Single-beat recording with no need for R-R interval matching	<ul style="list-style-type: none">• Unreliable when RA pressure is elevated
			
RV global systolic function FAC	RV FAC in RV-focused apical four-chamber view: $RV FAC (\%) = 100 \times (EDA - ESA)/EDA$	<ul style="list-style-type: none">• Established prognostic value• Reflects both longitudinal and radial components of RV contraction• Correlates with RV EF by CMR	<ul style="list-style-type: none">• Neglects the contribution of RV outflow tract to overall systolic function• Only fair inter-observer reproducibility
			
EF	Fractional RV volume change by 3D TTE: $RV EF (\%) = 100 \times (EDV - ESV)/EDV$	<ul style="list-style-type: none">• Includes RV outflow tract contribution to overall function• Correlates with RV EF by CMR	<ul style="list-style-type: none">• Dependent on adequate image quality• Load dependency• Requires offline analysis and experience• Prognostic value not established
			

Continued

Table 9 Continued				
Echocardiographic imaging				
RV longitudinal systolic function				
TAPSE		Recommended methods	Advantages	Limitations
		<ul style="list-style-type: none">• Tricuspid annular longitudinal excursion by M-mode (mm), measured between end-diastole and peak systole• Proper alignment of M-mode cursor with the direction of RV longitudinal excursion should be achieved from the apical approach.	<ul style="list-style-type: none">• Established prognostic value• Validated against radionuclide EF	<ul style="list-style-type: none">• Angle dependency• Partially representative of RV global function*
Pulsed tissue Doppler S wave		<ul style="list-style-type: none">• Peak systolic velocity of tricuspid annulus by pulsed-wave DTI (cm/sec), obtained from the apical approach, in the view that achieves parallel alignment of Doppler beam with RV free wall longitudinal excursion	<ul style="list-style-type: none">• Easy to perform• Reproducible• Validated against radionuclide EF• Established prognostic value	<ul style="list-style-type: none">• Angle dependent• Not fully representative of RV global function, particularly after thoracotomy, pulmonary thromboendarterectomy or heart transplantation
				
Color tissue Doppler S wave		<ul style="list-style-type: none">• Peak systolic velocity of tricuspid annulus by color DTI (cm/sec)	<ul style="list-style-type: none">• Sampling is performed after image acquisition• Allows multisite sampling on the same beat	<ul style="list-style-type: none">• Angle dependent• Not fully representative of RV global function, particularly after thoracotomy, pulmonary thromboendarterectomy or heart transplantation• Lower absolute values and reference ranges than pulsed DTI S' wave• Requires offline analysis• Vendor dependent
				
GLS		<ul style="list-style-type: none">• Peak value of 2D longitudinal speckle tracking derived strain, averaged over the three segments of the RV free wall in RV-focused apical four-chamber view (%)	<ul style="list-style-type: none">• Angle independent• Established prognostic value	
				

EDA, End-diastolic area; ESA, end-systolic area; ET, ejection time; GLS, gold longitudinal strain; IVCT, isovolumic contraction time; TCO, tricuspid valve closure—to–opening time.

EDA, End-diastolic area; ESA, end-systolic area; ET, ejection time; GLS, gold longitudinal strain; IVCT, isovolumic contraction time; TCO, tricuspid valve closure-to-opening time.

8. RV Systolic Function

RV systolic function has been evaluated using multiple parameters (Table 9), including RIMP, TAPSE, 2D FAC, 3DEEF, S', and longitudinal strain and strain rate by DTI and 2D STE.²⁵ Multiple studies have demonstrated the clinical utility and value of RIMP, TAPSE, 2D FAC, and S' of the tricuspid annulus, as well as longitudinal speckle-tracking echocardiographic strain. RV EF by 3DE seems to be more reliable and have better reproducibility when properly performed,

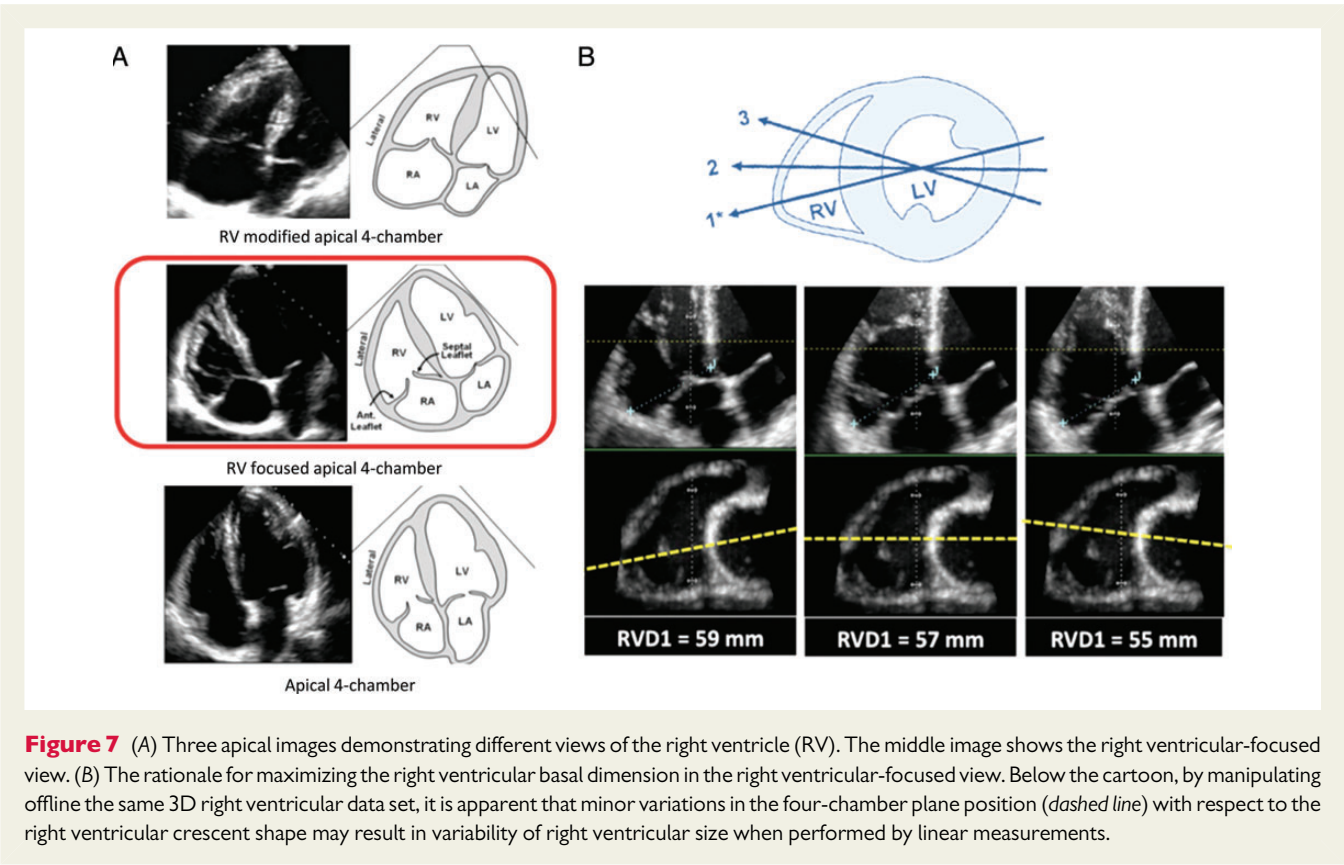
and a growing body of data are currently available to provide normal reference values (Table 10 and Supplemental Table 8).

8.1 RIMP

RIMP is an index of global RV performance. The isovolumic contraction time, the isovolumic relaxation time, and ejection time intervals should be measured from the same heartbeat using either PW spectral Doppler or DTI velocity of the lateral tricuspid annulus (Table 9).

Table 10 Normal values for parameters of RV function		
Parameter	Mean ± SD	Abnormality threshold
TAPSE (mm)	24 ± 3.5	<17
Pulsed Doppler S wave (cm/sec)	14.1 ± 2.3	<9.5
Color Doppler S wave (cm/sec)	9.7 ± 1.85	<6.0
RV fractional area change (%)	49 ± 7	<35
RV free wall 2D strain* (%)	−29 ± 4.5	> −20 (<20 in magnitude with the negative sign)
RV 3D EF (%)	58 ± 6.5	<45
Pulsed Doppler MPI	0.26 ± 0.085	>0.43
Tissue Doppler MPI	0.38 ± 0.08	>0.54
E wave deceleration time (msec)	180 ± 31	<119 or >242
E/A	1.4 ± 0.3	<0.8 or >2.0
e'/a'	1.18 ± 0.33	<0.52
e'	14.0 ± 3.1	<7.8
E/e'	4.0 ± 1.0	>6.0

MPI, Myocardial performance index.
* Limited data; values may vary depending on vendor and software version.



When using PW spectral Doppler to calculate RIMP, it important to ensure that the nonconsecutive beats have similar RR intervals. This limitation does not apply to the DTI-based RIMP measurements. RIMP can be falsely low in conditions associated with elevated RA pressures, which will shorten the IVRT. RIMP >0.43 by PW Doppler and >0.54 by DTI indicate RV dysfunction.

8.2 TAPSE
TAPSE is easily obtainable and represents a measure of RV longitudinal function. It is measured by M-mode echocardiography with the cursor optimally aligned along the direction of the tricuspid lateral annulus in the apical four-chamber view (Table 9). Although this index predominantly reflects RV longitudinal function, it has shown

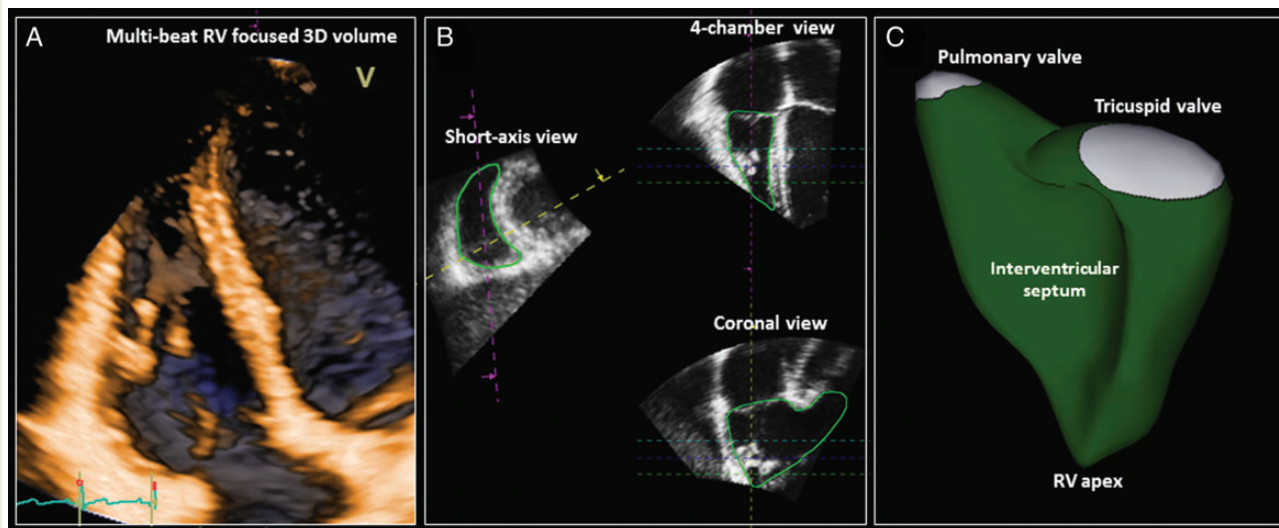


Figure 8 Three-dimensional analysis of the right ventricle (RV). (A) A 3D data set is acquired from a right ventricular-focused apical four-chamber view by stitching together the subvolumes generated from several (four to six) consecutive beats. (B) The right ventricular endocardial surface is semiautomatically identified after manual initialization in the right ventricular short-axis, four-chamber, and coronal views in both end-systole and end-diastole. (C) The generated 3D surface model of the RV enables the quantitation of right ventricular ESV and EDV, stroke volume, and EF.

good correlations with parameters estimating RV global systolic function, such as radionuclide-derived RV EF, 2D echocardiographic RV FAC, and 2D echocardiographic EF. As a one-dimensional measurement relative to the transducer position, TAPSE may over- or underestimate RV function because of cardiac translation.⁷⁹ Although there may be minor variations in TAPSE values according to gender and BSA, generally, TAPSE < 17 mm is highly suggestive of RV systolic dysfunction.

8.3 RV 2D FAC

FAC provides an estimate of global RV systolic function. It is important to ensure that the entire right ventricle be contained in the imaging sector, including the apex and the free wall, during both systole and diastole. While tracing the RV area, care must be taken to include the trabeculae in the RV cavity (Table 9). RV FAC < 35% indicates RV systolic dysfunction.

8.4 DTI-Derived Tricuspid Lateral Annular Systolic Velocity

DTI-derived S'-wave velocity is easy to measure, reliable, and reproducible, and it has been shown to correlate well with other measures of global RV systolic function. Specific age-related cutoff values have been reported in a large sample of healthy subjects.⁸⁰ It is important to keep the basal segment and the annulus aligned with the Doppler cursor to avoid velocity underestimation (Table 9). Similar to TAPSE, S' is measured relative to the transducer and may therefore be influenced by overall heart motion. An S' velocity < 9.5 cm/sec measured on the free-wall side indicates RV systolic dysfunction.

8.5 RV Strain and Strain Rate

Strain and strain rate are useful parameters for estimating RV global and regional systolic function. Longitudinal strain is calculated as the percentage of systolic shortening of the RV free wall from base

to apex, while longitudinal strain rate is the rate of this shortening. RV longitudinal strain is less confounded by overall heart motion^{79,81} but depends on RV loading conditions as well as RV size and shape. RV longitudinal strain should be measured in the RV-focused four-chamber view. Compared with STE-derived strain, the angle dependency of DTI strain is a disadvantage. RV speckle-tracking echocardiographic strain is influenced by image quality, reverberation and other artifacts, as well as attenuation. Placing the basal reference points too low (i.e., on the atrial side of the tricuspid annulus) might result in artifactually low basal strain values. The width of the region of interest should be limited to the myocardium, excluding the pericardium, which may be difficult given the usually thin RV free wall (Table 9).

In the context of the right ventricle, GLS is a parameter borrowed from LV measurements, and software currently used to measure RV GLS from most manufacturers has been designed for LV measurements and later adapted for the right ventricle. The term RV GLS usually refers to either the average of the RV free wall and the septal segments or the RV free wall segments alone (Figure 9). Peak global longitudinal RV strain excluding the interventricular septum has been recently reported to have prognostic value in various disease states, such as heart failure,^{82,83} acute myocardial infarction,⁸⁴ pulmonary hypertension,^{85,86} and amyloidosis,⁸⁷ and to predict RV failure after LV assist device implantation.⁸⁸

The largest body of evidence comes from the single-center studies cited above, which involved predominantly imaging equipment and software from two vendors, where pooled data were derived from limited number of subjects. Current reference values for global RV free wall speckle-tracking echocardiographic strain are reported in Table 10. Pooled data (though heavily weighted by a single vendor) suggest that global longitudinal RV free wall strain > -20% (i.e., < 20% in absolute value) is likely abnormal.

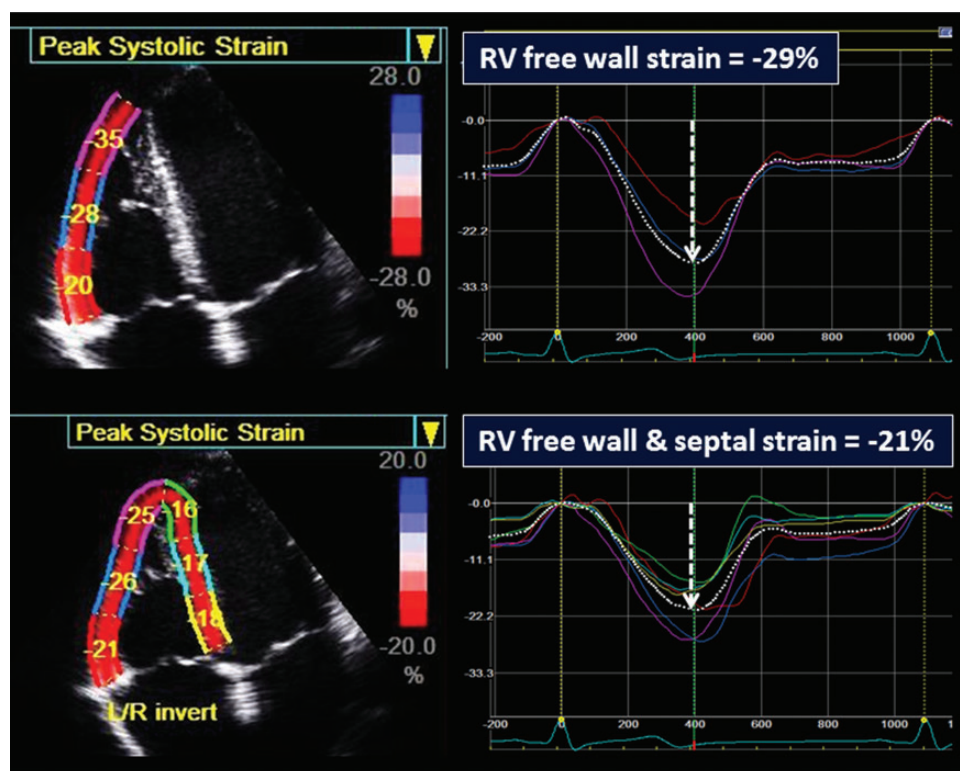


Figure 9 Measurement of RV systolic strain by 2D STE. The upper panel demonstrates RV “global” free wall strain whereby the three segments of the free wall are averaged, and the lower panel demonstrates “global” longitudinal strain of the six segments of the apical four-chamber view: three free wall and three septal segments. Note that RV longitudinal strain is significantly higher (as an absolute value) than the strain averaged from both septal and free wall segments. Until a universal standard is established, the interpretation of RV longitudinal strain values should take into account the methodology and vendor- and method-specific reference values.

Recommendations

Two-dimensional STE-derived strain, particularly of the RV free wall, appears to be reproducible and feasible for clinical use. Because of the need for additional normative data from large studies involving multi-vendor equipment, no definite reference ranges are currently recommended for either global or regional RV strain or strain rate.

8.6 RV 3D EF

Three-dimensional echocardiographic RV EF is a global measure of RV systolic performance. Although RV EF does not directly reflect RV contractile function per se, it provides an integrated view of the interaction between RV contractility and load. RV EF can be of particular clinical value in patients after cardiac surgery (in the absence of marked septal shift), when conventional indices of longitudinal RV function (i.e., TAPSE, S' wave) are generally reduced and no longer representative of overall RV performance.^{81,89,90} Three-dimensional echocardiography has been extensively validated against CMR,^{78,91} and the volumetric semiautomated border detection approach is the recommended method for the assessment of RV EF.

The limitations of 3D assessment of RV EF are load dependency, interventricular changes affecting septal motion, poor acoustic windows, and irregular rhythms. As described above in the section

on RV volume, the RV EF is slightly higher in women than in men, because of smaller volumes, and it is recommended to refer to gender-specific values (Supplemental Table 8).

Recommendation

In laboratories with appropriate 3D platforms and experience, 3DE-derived RV EF should be considered as a method of quantifying RV systolic function, with the limitations mentioned above. Roughly, an RV EF of <45% usually reflects abnormal RV systolic function, though laboratories may choose to refer to age- and gender-specific values.

III. The Left and Right Atria

The left atrium fulfills three major physiologic roles that influence LV filling and performance. The left atrium acts as a (1) contractile pump that delivers 15% to 30% of the entire LV filling, (2) reservoir that collects pulmonary venous return during ventricular systole, and (3) conduit for the passage of stored blood from the left atrium to the left ventricle during early ventricular diastole.^{92,93} An enlarged left atrium is associated with adverse cardiovascular outcomes.^{94–99} In the absence of mitral valve disease, an increase in LA size most commonly reflects increased wall tension as a result of increased LA

pressure,^{100–103} as well as impairment in LA function secondary to an atrial myopathy.^{104,105} A clear relationship exists between an enlarged left atrium and the incidence of atrial fibrillation and stroke,^{92,106–115} risk for overall mortality after myocardial infarction,^{104,105,116,117} risk for death and hospitalization in patients with dilated cardiomyopathy,^{118–122} and major cardiac events or death in patients with diabetes mellitus.¹²³ LA enlargement is a marker of both the severity and chronicity of diastolic dysfunction and magnitude of LA pressure elevation.^{98,100–103}

9. LA Measurements

9.1 General Considerations for LA Size

TTE is the recommended approach for assessing LA size. Recommendations for LA quantification are summarized in *Table 11*. With TEE, the entire left atrium frequently cannot be fit in the image sector. Accordingly, TEE should not be used to assess LA size. LA size should be measured at the end of LV systole, when the LA chamber is at its greatest dimension. While acquiring images to measure LA size and volumes, care should be taken to avoid foreshortening of the left atrium. Because the longitudinal axes of the left ventricle and left atrium frequently lie in different planes, dedicated acquisitions of the left atrium from the apical approach should be obtained for optimal LA volume measurements. The base of the left atrium should be at its largest size, indicating that the imaging plane passes through the maximal short-axis area. LA length should also be maximized to ensure alignment along the true long axis of the left atrium. When using the biplane disk summation method to calculate LA volumes, the lengths of the long axes measured in the two- and four-chamber views should be similar. When tracing the borders of the left atrium, the confluences of the pulmonary veins and the LA appendage should be excluded. The atrioventricular interface should be represented by the mitral annulus plane, not by the tip of the mitral leaflets.

9.2 Linear Dimensions and Area Measurements

The most widely used linear dimension is the LA anteroposterior (AP) measurement in the parasternal long-axis view using M-mode echocardiography or, preferably, 2DE.^{92,107,109,110,114,118,120,121,124,125} Although this measurement has been used extensively in clinical practice and research, it has become clear that frequently it may not represent an accurate picture of LA size.^{126,127} Traditionally, the AP dimension was widely used because it was known to be the most reproducible measurement. However, assessment of LA size using only the AP diameter assumes that when the left atrium enlarges, all its dimensions change similarly, which is often not the case during LA remodeling.^{128–130} Therefore, AP linear dimension should not be used as the sole measure of LA size. LA area can be planimetered in the apical four- and two-chamber views and normal values for these parameters have been reported.¹² Optimal contours should be obtained orthogonally around the long axis of the left atrium from good quality images while avoiding foreshortening.¹ The ease with which LA volumes can be obtained in clinical practice in conjunction with the existing robust literature on normal values and the prognostic value of LA volumes renders reporting of LA area unnecessary.

9.3 Volume Measurements

When assessing the LA size and remodeling, the measurement of LA volume is recommended. Evaluation of volume takes into account alterations in LA chamber size in all directions. LA volume has been shown to be a powerful prognostic variable in a variety of cardiac disease states.^{99,106,112,113,115–117,122,131–136} Compared with AP diameter, LA volume has a stronger association with outcomes in cardiac patients.^{113,137} Two-dimensional echocardiographic LA volumes are typically smaller than those reported from computed tomography or CMR.^{138–142} Measurements of LA volumes are important, because they reflect the burden and chronicity of elevated LV filling pressures and are a strong predictor of outcomes.

Different methods exist for measuring LA volumes. Although the three linear measurements have been used to calculate LA volume using an ellipsoid model,^{131,137,143} the relative inaccuracy of these linear measurements limits this method. LA volume should be measured using the disk summation algorithm, similar to that used to measure LV volume (*Table 11*).^{144,145}

The LA endocardial borders should be traced in both the apical four- and two-chamber views. A single-plane approach can also be used, but this method is based on the geometric assumption that the left atrium is circular in the short-axis cut plane, which may not be always accurate.¹⁴⁶ Although not recommended for routine use, this approach could be used in cases when planimetry in both views is difficult. Single-plane apical four-chamber indexed LA volumes are typically 1 to 2 mL/m² smaller than apical two-chamber volumes.^{12,146}

Alternatively, a biplane calculation could also be performed using the LA areas and lengths measured from both the apical four- and two-chamber views (*Table 11*). Although the area-length method still assumes an ellipsoidal LA shape, it has the advantage of reducing linear dimensions to only two measurements of atrial length, of which the shorter one is selected.^{98,147}

9.4 Normal Values of LA Measurements

Since the publication of the 2005 chamber quantification guidelines, two articles have reported normal values for LA linear measurements.^{12,143} These values were in keeping with prior recommendations, and accordingly, no modifications have been made to the normal values of LA AP diameters (*Supplemental Table 9*). Although not recommended for routine clinical use, normal values for apical four- and two-chamber linear measurements and nonindexed LA area and volume measurements have been reported.¹²

LA size is dependent on gender. However the gender differences in LA size are generally accounted for when adjusting for body size.¹² Several indexing methods have been proposed,^{137,148} but indexing to BSA has yielded the most available data and is recommended by the writing group. Indexing by BSA accounts for the gender differences in LA size, such that only the indexed value should be reported.^{93,137,149,150}

In the prior chamber quantification guideline document, the reported BSA-indexed LA volume normal values were based on two studies performed in a small number of subjects.^{98,144} Since the publication of that document, eight additional studies (1,234 patients) describing normal values of LA volumes using the area-length ellipsoid or the disk summation techniques have been reported.^{11,12,145,147,151–155} This has resulted in a change in the

Volume

2D volumetric measurements are based on tracings of the blood-tissue interface on apical four- and two-chamber views. At the mitral valve level, the contour is closed by connecting the two opposite sections of the mitral annulus with a straight line. Endocardial tracing should exclude atrial appendage and pulmonary veins. LA length L is defined as the shortest of the two long axes measured in the apical two- and four-chamber views (to provide reliable calculations the two lengths should not differ more than 5 mm). Volumes can be computed by using the area-length approximation:

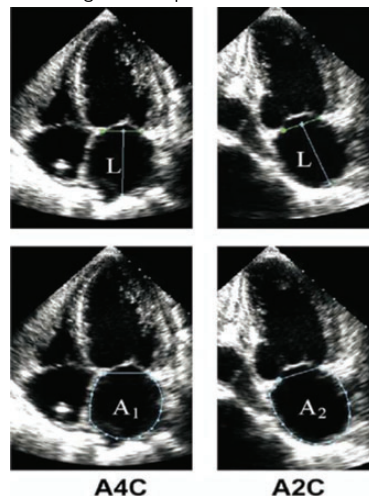
$$\frac{8}{3\pi} \left[\frac{(A_1 \cdot A_2)}{L} \right]$$

where A1 and A2 are the corresponding LA areas. Alternatively LA volume can be calculated using the disk summation technique by adding the volume of a stack of cylinders of height h and area calculated by orthogonal minor and major transverse axes (D1 and D2) assuming an oval shape:

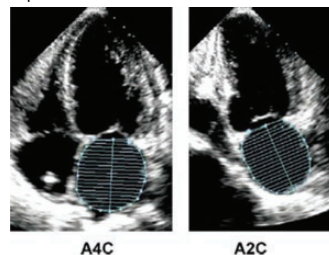
$$\pi/4(h) \sum (D1)(D2)$$

3D data sets are usually obtained from the apical approach using a multibeam full-volume acquisition

2DE Area-length technique



Biplane method of disks



3D data sets



- Enables accurate assessment of the asymmetric remodeling of the left atrium
- More robust predictor of cardiovascular events than linear or area measurements
- Geometric assumptions about LA shape
- Few accumulated data on normal population
- Single plane volume calculations are inaccurate since they are based on the assumption that $A1 = A2$
- No geometrical assumption about LA shape
- More accurate when compared to 2D measurements
- Dependent on adequate image quality
- Lower temporal resolution
- Limited data on normal values
- Patient's cooperation required

recommended upper normal indexed LA volume to 34 mL/m² (previously 28 mL/m²). In addition, LA volume data became available in 1,331 patients from the five databases described earlier in this document, wherein the mean calculated LA volume was 25 mL/m². This upper normal revised value of 34 mL/m² also seems to fit in well with a risk-based approach for determination of cutoffs between a normal and an enlarged left atrium.^{106,123,134,136} This cutoff value is also consistent with the ASE and European Association of Echocardiography guideline document on evaluation of diastolic function.¹⁵⁶ The 2DE-derived biplane LA volumes are listed in Table 4, including normal ranges and severity partition cutoffs. Of note, LA volume can be increased in elite athletes, which needs to be taken into account to avoid misinterpretation as abnormal.¹⁴⁶

Three-dimensional echocardiography holds promise for assessing LA volume and correlates with cardiac computed tomography^{157,158} and magnetic resonance imaging.^{159,160} Compared with 2D assessment of LA volume, 3DE is more accurate compared with CMR^{159,160} and has superior prognostic ability.^{161,162} Three-dimensional echocardiographic LA volumes are typically larger than 2D echocardiographic volumes in most studies.^{160,163} Despite these advantages, the lack of a standardized methodology and limited normative data¹⁶⁴ prevent this committee from recommending the use of 3D echocardiographic normal values at this time.

Recommendations

Because it is theoretically more accurate than the area-length method, the biplane disk summation technique, which incorporates fewer geometric assumptions, should be the preferred method to measure LA volume in clinical practice. The upper normal limit for 2D echocardiographic LA volume is 34 mL/m² for both genders.

10. Right Atrial measurements

Less research and fewer clinical outcomes data are available on the quantification of RA size. Although the right atrium can be assessed from different views, quantification of RA size is most commonly performed from the apical four-chamber view (Table 12). The minor-axis dimension should be taken from a plane perpendicular to the long axis of the right atrium, extending from the lateral border of the right atrium to the interatrial septum. In contrast to the left atrium, RA size appears to be gender dependent, but prior ASE guidelines did not have sufficient data to provide normative data by gender.^{1,71} Recent data obtained from three cohorts of >2,400 patients now provide normal values of RA dimensions for men and women.^{12,73,165}

As with the left atrium, RA volumes are likely to be more robust and accurate for determination of RA size compared with linear dimensions. At the time of the prior guideline document, limited data were available for the determination of normative RA volumes. Because there are no standard orthogonal RA views to use for an apical biplane calculation, a single-view area-length and/or disk summation techniques has been proposed for RA volume determination.^{150,153,165–167} Of note, normal RA volumes for men are slightly larger than those for women, with indexing to BSA failing to equalize values between genders for reasons that are not fully understood.^{150,165} Recommendations for RA volume normative data are made from the two largest most contemporary data sets^{12,165} (Table 13). RA volumes are underestimated with 2D

echocardiographic techniques compared with 3DE.^{164,165,168} RA volumes in adult subjects appear to be smaller than LA volumes.^{12,150,153,165} This is because the RA volumes were obtained using a single-plane method of disks, in contrast to the LA volumes, which were established using the biplane technique.

Recommendations

The recommended parameter to assess RA size is RA volume, calculated using single-plane area-length or disk summation techniques in a dedicated apical four-chamber view. The normal ranges for 2D echocardiographic RA volume are 25 ± 7 mL/m² in men and 21 ± 6 mL/m² in women.

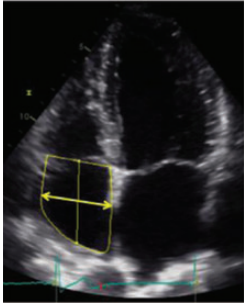
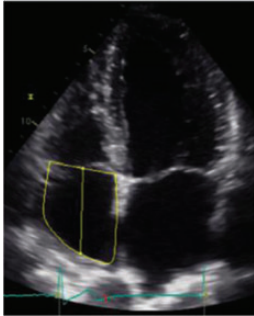
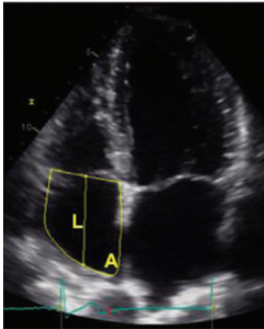
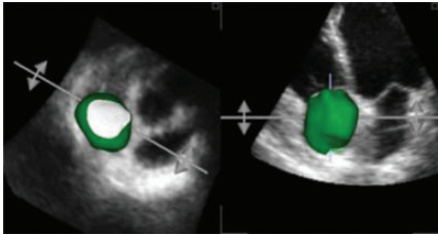
IV. The Aortic Annulus and Aortic Root

Detailed knowledge and quantification of the aortic root and aortic valve morphology has become even more crucial with the increasing use of transcatheter aortic valve implantation (TAVI) and transcatheter aortic valve replacement (TAVR) procedures. This knowledge is critically important for preprocedural planning, intraprocedural guidance, and postprocedural assessment.

The aortic root extends from the basal attachments of the aortic valve leaflets within the LV outflow tract to their distal attachment at the tubular portion of the aorta (the sinotubular junction).¹⁶⁹ The aortic root is a geometrically complex structure that includes (1) the aortic valve annulus, (2) the interleaflet triangles, (3) the semilunar aortic leaflets and their attachments, (4) the aortic sinuses of Valsalva, and (5) the sinotubular junction.^{170–172} Aortic measurements should be made at the following sites: (1) the aortic valve annulus, (2) the maximal diameter of the sinuses of Valsalva, (3) the sinotubular junction (usually a demarcated transition between the sinuses of Valsalva and the tubular portion of the ascending aorta), and (4) the maximal diameter of the proximal ascending aorta, including a notation of the distance between the measurement site and the sinotubular junction (Figure 10A).

11. The Aortic Annulus

The “aortic annulus” is not a true or distinct anatomic structure but is a virtual ring that may be defined by joining the basal attachments, or nadirs, of the three aortic leaflets. The distal (uppermost) attachments of the leaflets, in the shape of a crown, form a true anatomic ring.^{169,173} (Figure 10B). Approximately two-thirds of the circumference of the lower part of the aortic root is attached to the muscular interventricular septum, while the remaining one-third is in fibrous continuity with the anterior mitral valve leaflet.¹⁷⁴ Measurement of the aortic valve annulus before TAVI or TAVR is a challenge, and the ideal modality for its measurement has yet to be established. During the initial TAVI and TAVR experience, aortic annular measurements were routinely performed using 2DE.^{174,175} Although the standard approach during the early years of TAVI and TAVR was echocardiography using a one-dimensional measurement, this method has clear limitations for TAVI and TAVR valve sizing. At present, the two most commonly used imaging techniques used for measuring the aortic annulus before TAVI or TAVR are echocardiography and multidetector computed tomography (MDCT).

Parameter and method	Echocardiographic imaging	Advantages	Limitations
Linear dimensions The minor axis of the right atrium should be measured in the apical four-chamber view as the distance between the lateral RA wall and interatrial septum, at the midatrial level defined by half of RA long axis	2D-guided linear measurements 	<ul style="list-style-type: none">• Easy to obtain• Established normal values	<ul style="list-style-type: none">• Single dimension only• Assumes that RA enlargement is symmetrical• View dependent
Area Measured in the apical four-chamber view at end-systole, on the frame just prior to tricuspid valve opening, by tracing the RA blood-tissue interface, excluding the area under the tricuspid valve annulus.	2D view 	<ul style="list-style-type: none">• More representative of actual RA size than linear dimensions• Established normal values	<ul style="list-style-type: none">• Need of a dedicated view to avoid RA foreshortening• Assumes a symmetrical shape of the cavity• View dependent
Volume 2D volumetric measurements are usually based on tracings of the blood-tissue interface on the apical four-chamber view. At the tricuspid valve level, the contour is closed by connecting the two opposite sections of the tricuspid ring with a straight line. Volumes can be computed by using either the single plane area-length: $\frac{8}{3\pi} \left[\frac{(A_1)^2}{L} \right]$ or the disks summation technique. 3D data sets are usually obtained from the apical approach using a full-volume acquisition	2D view  3D data sets 	<ul style="list-style-type: none">• More representative of actual RA size than linear dimensions• No geometrical assumption• Established normal values	<ul style="list-style-type: none">• Assumes a symmetrical shape of the cavity• Single plane volume calculation may be inaccurate since it assumes that RA enlargement is symmetrical• Normal values not well established• Dependent on image quality• Lower temporal resolution• Patient's cooperation required

With echocardiography, measurements of the aortic annulus should be made in the zoom mode using standard electronic calipers in midsystole, when the annulus is slightly larger and rounder than in diastole, between the hinge points of the aortic valve leaflets (usually

between the hinge point of the right coronary cusp and the edge of the sinus at the side of the commissures between the left coronary cusp and the noncoronary cusp) from inner edge to inner edge. All other aortic measurements should be made at end-diastole, in a

Table 13 Normal RA size obtained from 2D echocardiographic studies

	Women	Men
RA minor axis dimension (cm/m ²)	1.9 ± 0.3	1.9 ± 0.3
RA major axis dimension (cm/m ²)	2.5 ± 0.3	2.4 ± 0.3
2D echocardiographic RA volume (mL/m ²)	21 ± 6	25 ± 7

Data are expressed as mean ± SD.

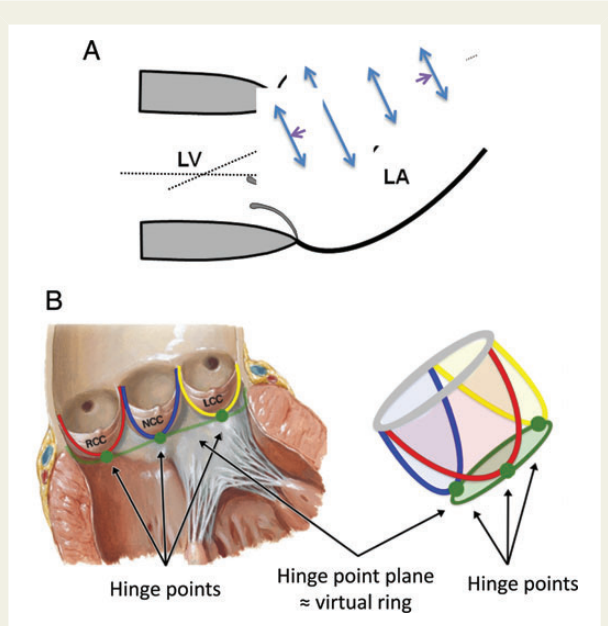


Figure 10 (A) Sites for measurements of the aortic root and ascending aorta. This diagram illustrates the four sites at which measurements are recommended (light blue arrows): (1) the aortic valve annulus (hinge point of aortic leaflets), (2) the sinuses of Valsalva (maximal diameter, usually the midpoint), (3) the sinotubular junction, and (4) the proximal ascending aorta (the distance between the measurement site and the annular plane [purple arrowheads] should always be reported). The aortic annulus should be measured at peak systole, in contrast to the other dimensions, which are measured at end-diastole. The dashed lines, depicting the longitudinal axis of the left ventricle (LV) and that of the aortic root and proximal ascending aorta, are different. Note that the angle between these two axes varies from individual to individual and with age and pathology. (B) Normal anatomy of the aortic annulus. The aortic annulus accounts for the tightest part of the aortic root and is defined as a virtual ring (shaded) with three anatomic anchor points at the nadir of each of the attachments of the three aortic leaflets. Reproduced with permission from Kasel et al.¹⁸⁴ Ao, Aorta; LA, left atrium.

strictly perpendicular plane to that of the long axis of the aorta. Aortic annular measurements may be difficult in patients with acoustic blooming caused by a calcified aortic annulus.^{176–179} As a general rule, calcium protuberances should be considered as part of the lumen, not of the aortic wall, and therefore excluded from the diameter measurement.

The anteroposterior diameter is commonly measured by both 2D TTE (from the parasternal long-axis view) and 3D TEE (from the longitudinal view of the proximal aortic root, usually 110°–130°) and approximates the minor dimension of the annulus measured by MDCT.^{3,176,180} However, because the annulus is often elliptical, with variable diameters, it is preferable to measure the annulus in a cross-sectional view, using 3D imaging, as recommended by the European Association of Echocardiography and ASE guidelines,¹⁸¹ the American College of Cardiology Foundation, American Association for Thoracic Surgery, Society for Cardiac Angiography and Interventions, and Society of Thoracic Surgeons consensus document on TAVR;¹⁸² the Society of Cardiovascular Computed Tomography expert consensus document on MDCT;¹⁸³ and others.^{184–187} Using 3D TEE, both the smaller (anteroposterior, sagittal) and larger (medial-lateral, coronal) diameters, as well as the perimeter and annular area, should be measured in a cross-sectional view in midsystole (Figure 11). It should be noted that the difference between major and minor diameters may be up to 6 mm.^{173,188–193} For a detailed, step-by-step approach to making these measurements using 3D TEE, which is beyond the scope of this document, the reader is referred to four recent publications.^{184–187} By using these techniques, close agreement with MDCT can be achieved.^{184,185}

It should be noted that proponents of each of the two modalities (3D TEE and MDCT) tout advantages. In fact, each of these methods has certain strengths and limitations. Limitations of MDCT include the need for contrast media, radiation exposure, inability to obtain real-time measurements during the procedure, and the need to control the heart rate for suitable gating. Three-dimensional TEE also has limitations. First, the software required to use the methodology described by Kasel et al.¹⁸⁴ and Pershad et al.¹⁸⁵ is not currently available on all echocardiographic platforms. Second, visualization of the anterior portion of the annulus can be obscured by echo “dropout” due to annular calcification. In addition, calcification at the level of the annulus may hinder the ability to determine boundary definition and may make its shape irregular. Third, the plane formed by the nadirs of the three cusps is often not orthogonal to the LV outflow tract or aortic root; frequently the insertion of the right coronary cusp is inferior to that of the left and noncoronary cusps.¹⁸³ Fourth, both the spatial and temporal resolution of 3D echocardiography is currently limited. Last, this technique is operator dependent and may be difficult at times, even in experienced hands.^{173,174} Because of these potential limitations, it is desirable to use a multi-modality approach for aortic annular measurement.

12. The Aortic Root

With 2D TTE, the diameter of the aortic root (at the maximal diameter of the sinuses of Valsalva) should be obtained from the parasternal long-axis view, which depicts the aortic root and the proximal ascending aorta. This plane is slightly different from that of the long axis of the left ventricle (Figure 10A). Acquisition of this LV long-axis view may be performed from different intercostal spaces and at various distances from the left sternal border. Use of simultaneous biplane orthogonal images provided by matrix transducers may be helpful. The tubular ascending aorta is often not adequately visualized from a standard parasternal window. In these instances, moving the transducer closer to the sternum may allow visualization of a longer portion of the ascending aorta. In addition, the ascending

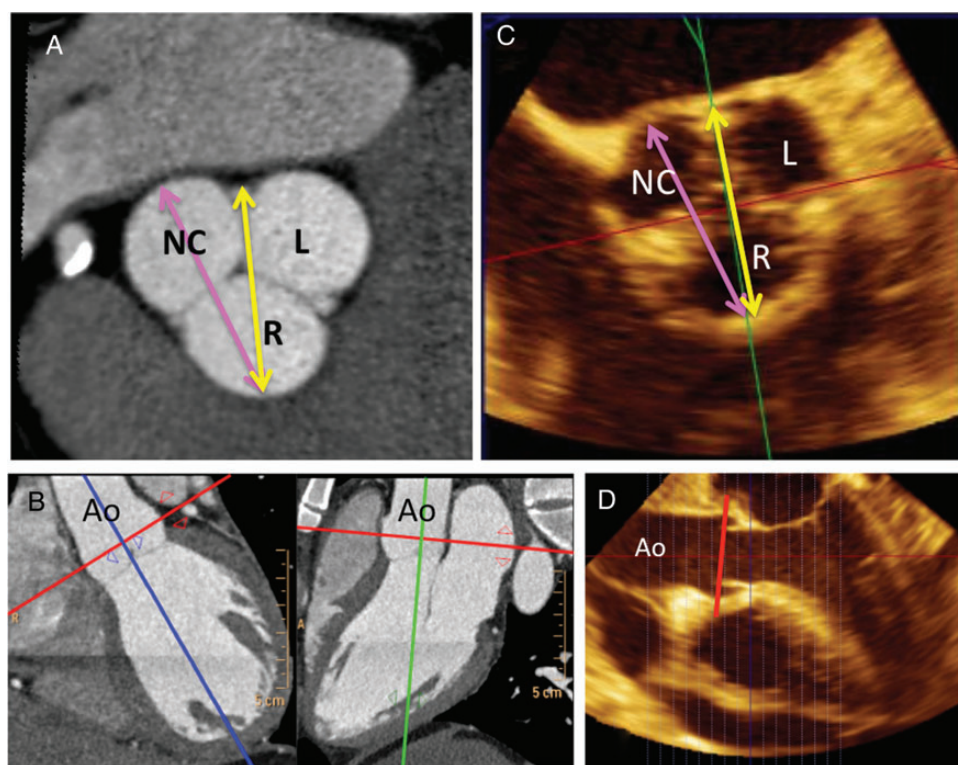


Figure 11 The smaller (antero-posterior, sagittal) aortic root diameter is measured using CT (A) or 3D TEE (C, zoomed cross sectional view) between the inner edges of the left (L) and non-coronary (NC) commissure to the opposite right (R) coronary sinus (A and C, yellow double arrows). The larger diameter (medial-lateral) is measured from the middle of the right sinus to the most distal point of the NC sinus (A and C, purple double arrows). Panel B shows zoomed cross-sectional CT views of aortic root at the sinus of Valsalva level using a double oblique image for orientation. Panel D shows a long-axis view of the aorta in obtained by multiplanar reconstruction. The red lines in (B) and (D) represent the planes from which the diameter of the aortic root should be measured at the level of the sinuses of Valsalva.

aorta may sometimes be well visualized from right parasternal windows in the second or third intercostal space, especially when the aorta is dilated.

Measurements should be made in the view that depicts the maximum aortic diameter perpendicular to the long axis of the aorta. In patients with tricuspid aortic valves, the closure line of the leaflets (typically the right coronary cusp and the noncoronary cusp) is in the center of the aortic root lumen, and the closed leaflets are seen on the aortic side of a line connecting the hinge points of the two visualized leaflets. An asymmetric closure line, in which the tips of the closed leaflets are closer to one of the hinge points, is an indication that the cross-section is not encompassing the largest root diameter (Figure 12).

Unfortunately, there is no uniform method of measurement of the aortic root and aorta. Echocardiography uses the leading edge-to-leading edge (L-L) convention, but other techniques, such as MDCT and CMR, use the inner edge-to-inner edge (I-I) or outer edge-to-outer edge convention. In the consensus document,¹⁹⁴ the ASE and EACVI writing committee took the initiative to provide a common standard for measurement of the aortic root and aorta by recommending a switch to the I-I convention for echocardiography. However, this goal of achieving uniformity among modalities was ultimately abandoned for several reasons. First, currently used

long-standing reference values for the aorta were obtained using the L-L convention.^{195,196} Second, the L-L convention provides statistically larger diameters than the I-I convention (by 2–4 mm), and switching to the I-I convention raised a concern that patients at potential risk for developing life-threatening complications such as aortic dissection and/or rupture would fall below a threshold for intervention recommendation by current guidelines. Accordingly, the aortic annulus should be measured using the I-I convention, but we continue to recommend the L-L convention for measurements of the aortic root and aorta.

Two-dimensional echocardiographic aortic diameter measurements are preferable to M-mode measurements, because cardiac motion may result in changes in the position of the M-mode cursor relative to the maximum diameter of the sinuses of Valsalva. This translational motion may result in systematic underestimation (by approximately 2 mm) of the aortic diameter by M-mode imaging in comparison with 2D echocardiographic measurements.¹⁹⁵ The thoracic aorta can be better imaged using TEE compared with the TTE approach, because that aortic segment is in the near field of the transesophageal echocardiographic transducer. The aortic root and ascending aorta can be best seen in the midesophageal aortic valve long-axis view (three-chamber view at about 120°–140°).³ The short-axis view of the ascending aorta is best obtained using

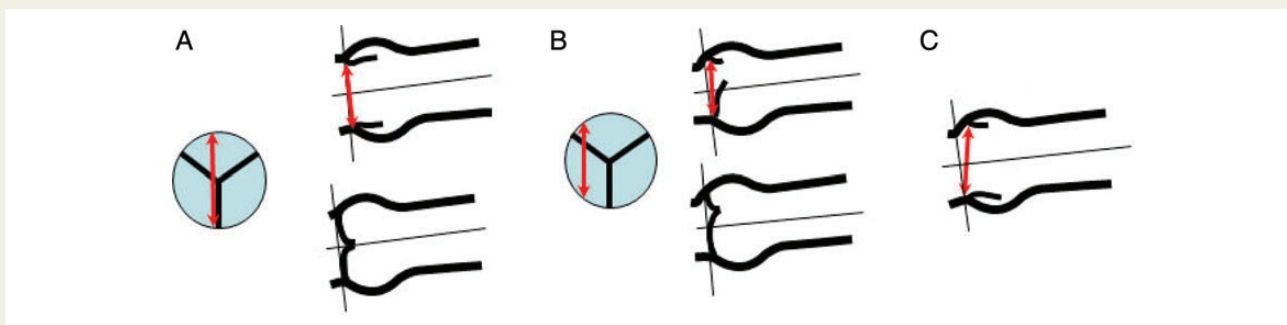


Figure 12 Correct (A) and incorrect (B, C) measurements of the aortic annulus (double arrows). (A) Centrally positioned diameter and central closure of leaflets. Thin lines correspond to the long axis of the ascending aorta and, orthogonally, to correct orientation of the annular diameter. (B) Incorrect, eccentric annular measurement. The hinge points are slightly displaced upward and do not correspond to the nadir of the cusp attachments, with incomplete opening and closing of leaflets. (C) Incorrect, oblique annular measurement. The annulus is “virtual” and only defined by the hinge-points of the three aortic valve leaflets. As such, much of the ring is without a visible anatomic structure. However, its location on any long-axis two-dimensional view can be approximated since the plane of the virtual annulus is approximately perpendicular to the long-axis of the aorta. When bisecting the maximum dimension of the annulus in the sagittal plane, one will image the right coronary cusp anteriorly and the fibrous trigone between the left and noncoronary cusps posteriorly. Because only one anatomic marker (the RCC hinge-point) is seen, the opposing annulus must be approximated with a measurement that is perpendicular to the long axis of the aorta. Attempting to measure what you believe to be 2 hinge-points (B and C) typically will measure within the sinuses of Valsalva and overestimate the annulus.

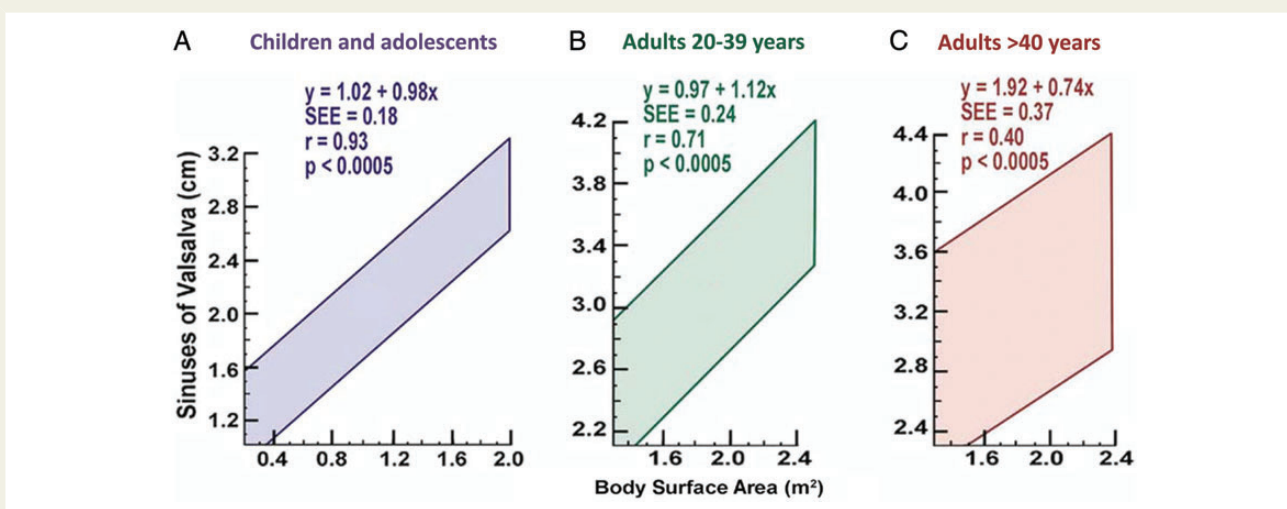


Figure 13 The 95% confidence intervals for aortic root diameter at sinuses of Valsalva on the basis of BSA in children and adolescents (A), adults aged 20 to 39 years (B), and adults aged ≥ 40 years (C). Reprinted with permission from Roman et al.¹⁹⁵

the midesophageal views at about 45° . For measurements of the descending aorta, short-axis views at about 0° and long-axis views at about 90° should be obtained from the level of the diaphragm up to the aortic arch. The biplane imaging function on current 3D echocardiographic imaging systems allows simultaneous visualization of both short- and long-axis views.

13. Identification of Aortic Root Dilatation

Aortic root dilatation is associated with the presence and progression of aortic regurgitation¹⁹⁷ and with the occurrence of aortic dissection. The presence of hypertension appears to have minimal impact on aortic root diameter at the level of the sinuses of Valsalva level¹⁹⁷ but is associated with enlargement of more distal aortic

segments. Aortic root diameter measurements at the level of the sinuses of Valsalva is closely related to BSA and age. Therefore, BSA may be used to predict aortic root diameter in three age strata, < 20 , 20 to 40, and > 40 years, by using published equations.¹⁹⁵ Aortic root dilatation at the sinuses of Valsalva is defined as an aortic root diameter above the upper limit of the 95% confidence interval of the distribution in a large reference population. Aortic dilatation can be easily detected by plotting observed aortic root diameter versus BSA on previously published nomograms (Figure 13).¹⁹⁵ Equations to determine the expected aortic diameter at the sinuses of Valsalva in relation to BSA for each of the three age strata are also shown in Table 14 and Figure 13. The aortic root index or ratio of observed to expected aortic root diameters can be calculated by dividing the observed by the expected diameter.

Table 14 Aortic root dimensions in normal adults

Aortic root	Absolute values (cm)		Indexed values (cm/m ²)	
	Men	Women	Men	Women
Annulus	2.6 ± 0.3	2.3 ± 0.2	1.3 ± 0.1	1.3 ± 0.1
Sinuses of Valsalva	3.4 ± 0.3	3.0 ± 0.3	1.7 ± 0.2	1.8 ± 0.2
Sinotubular junction	2.9 ± 0.3	2.6 ± 0.3	1.5 ± 0.2	1.5 ± 0.2
Proximal ascending aorta	3.0 ± 0.4	2.7 ± 0.4	1.5 ± 0.2	1.6 ± 0.3

Adapted from Roman et al.¹⁹⁵ and Hiratzka et al.²⁰⁴

Recommendations

The aortic annulus should be measured at midsystole from inner edge to inner edge. All other aortic root measurements (i.e., maximal diameter of the sinuses of Valsalva, the sinotubular junction, and the proximal ascending aorta) should be made at end-diastole, in a strictly perpendicular plane to that of the long axis of the aorta using the L-L convention. Measurements of maximal diameter of the aortic root at the sinuses of Valsalva should be compared with age- and BSA-related nomograms or to values calculated from specific allometric equations. Accurate measurement of the aortic annulus before TAVI or TAVR is crucial. To date, there is no established gold-standard technique for measuring the aortic annulus before TAVI or TAVR. Three-dimensional TEE and MDCT are emerging as reliable and possibly preferred methods for aortic annulus measurements.

V. The Inferior Vena Cava

Examination of the IVC from the subcostal view should be included as part of the routine transthoracic echocardiographic examination. It is generally agreed that the diameter of the IVC should be measured in the subcostal view with the patient in the supine position at 1.0 to 2.0 cm from the junction with the right atrium, using the long-axis view. For accuracy, this measurement should be made perpendicular to the IVC long axis. The diameter of the IVC decreases in response to inspiration when the negative intrathoracic pressure leads to an increase in RV filling from the systemic veins. The diameter of the IVC and the percentage decrease in the diameter during inspiration correlate with RA pressure. The relationship may be quantified as the collapsibility index.¹⁹⁸ Evaluation of the inspiratory response often requires a brief sniff, as normal inspiration may not elicit this response.

For simplicity and uniformity of reporting, specific values of RA pressure, rather than ranges, should be used in the determination of systolic pulmonary artery pressure. IVC diameter <2.1 cm that collapses >50% with a sniff suggests normal RA pressure of 3 mm Hg (range, 0–5 mm Hg), whereas IVC diameter >2.1 cm that collapses <50% with a sniff suggests high RA pressure of 15 mm Hg (range, 10–20 mm Hg).¹⁹⁹ In scenarios in which IVC diameter and collapse do not fit this paradigm, an intermediate value of 8 mm Hg (range, 5–10 mm Hg) may be used, or, preferably, other indices of RA pressure should be integrated to downgrade or upgrade to the normal or high values of RA pressure. It should be noted that in normal young athletes, the IVC may be dilated in the

presence of normal pressure.^{200,201} In addition, the IVC is commonly dilated and may not collapse in patients on ventilators, so it should not be routinely used in such cases to estimate RA pressure.²⁰² However, IVC diameter measured on TEE at the cavoatrial junction has been successfully used to derive central venous pressure in anesthetized mechanically ventilated patients.²⁰³ The use of the IVC size and dynamics is encouraged for estimation of RA pressure. This estimate should be used in estimation of the pulmonary artery pressure on the basis of the tricuspid regurgitant jet velocity, rather than assuming a constant RA pressure for all patients.

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Abbreviations

AP, Anteroposterior; ASE, American Society of Echocardiography; BSA, Body surface area; CMR, Cardiac magnetic resonance; DTI, Doppler tissue imaging; EACVI, European Association of Cardiovascular Imaging; EDV, End-diastolic volume; EF, Ejection fraction; ESV, End-systolic volume; FAC, Fractional area change; GLS, Global longitudinal strain; I-I, Inner edge-to-inner edge; IVC, Inferior vena cava; LA, Left atrial; L-L, Leading edge-to-leading edge; LV, Left ventricular; MDCT, Multidetector computed tomography; PW, Pulsed-wave; RA, Right atrial; RIMP, Right ventricular index of myocardial performance; RV, Right ventricular; RWT, Relative wall thickness; STE, Speckle-tracking echocardiography; TAPSE, Tricuspid annular plane systolic excursion; TAVI, Transcatheter aortic valve implantation; TAVR, Transcatheter aortic valve replacement; TEE, Transesophageal echocardiography; 3D, Three-dimensional; 3DE, Three-dimensional echocardiography; TTE, Transthoracic echocardiography; 2D, Two-dimensional; 2DE, Two-dimensional echocardiography

Supplementary data

Supplementary data are available at *European Heart Journal – Cardiovascular Imaging* online.

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