



# Drowsiness Detection using Machine Learning and Multiple Bio-Markers

Preetam Teja B, Sarvesh K, Durai Singh K and Samhitha S

School Of Computing, Amrita Vishwa Vidyapeetham, Ettimadai, 641112, Tamil Nadu, India

## Abstract

Recent research in drowsiness detection has primarily focused on deep learning (DL) models due to their high accuracy. However, these approaches often yield only marginal gains while demanding extensive data, computational resources, and complex training, limiting their real-world applicability. Moreover, DL models' lack of interpretability hinders clinical and safety-critical adoption. We propose a classical machine learning (ML) approach, featuring signal preprocessing, engineered feature extraction, and both linear and non-linear classification. Our results show that ML models can achieve comparable performance to DL while offering greater transparency and efficiency, making them a practical, resource-friendly solution for real-world drowsiness detection.

**Key words:** drowsiness detection, classical machine learning, interpretability, feature extraction, real-world application

## Introduction

Drowsiness detection has emerged as a crucial area of research due to its profound impact on both public safety and healthcare. As our society becomes increasingly dependent on tasks that require sustained attention and alertness, the dangers of drowsiness have become more apparent. For instance, drowsy driving remains a significant contributor to road accidents worldwide, leading to severe injuries, fatalities, and substantial economic costs. Similarly, sleep disorders that impair alertness are associated with numerous health risks, making the development of effective drowsiness detection mechanisms an urgent necessity (??).

Unlike traditional sleep stage classification, which is frequently utilized in clinical sleep studies to assess sleep quality and diagnose disorders, our research specifically addresses the detection of drowsiness. This focus is critical because drowsiness is not a static state but rather a fluid, progressive transition between wakefulness and sleep. Capturing this gradual change is essential for practical applications, as it can severely affect cognitive and motor performance. For example, when a driver begins to experience drowsiness, their reaction time, decision-making ability, and situational awareness deteriorate, increasing the likelihood of accidents. The same risks are evident in other high-stakes environments, such as the operation of heavy machinery or in healthcare settings where alertness is crucial (??).

The gold standard for assessing sleep and related physiological states is polysomnography (PSG). PSG provides a comprehensive monitoring setup, recording brain activity through electroencephalography (EEG), eye movements using electrooculography (EOG), muscle tone with electromyography (EMG), and sometimes additional measures like heart rate and breathing

patterns. This multi-faceted approach enables a detailed understanding of an individual's sleep architecture. However, interpreting PSG data is far from straightforward. Manual scoring of these signals is typically performed by trained sleep experts who follow established guidelines, such as those set by the American Academy of Sleep Medicine (AASM) (?). Despite these guidelines, the process is time-consuming, often taking hours to annotate a full night's sleep recording. Moreover, the manual scoring process is inherently subjective, leading to variability between different scorers (inter-scorer reliability) and even within the same scorer at different times (intra-scorer reliability). Research has documented inter-scorer agreement rates as low as 83

While the advent of deep learning has revolutionized many areas of medical data analysis, including sleep staging, these models come with their own set of challenges. Deep learning models have demonstrated impressive performance in automating the classification of sleep stages, but their practical utility in real-world clinical or safety-critical environments remains limited. One of the main issues is the high demand for large, annotated datasets. Training deep learning models effectively requires vast amounts of labeled data, which can be difficult to obtain and curate. Furthermore, these models are computationally expensive, often necessitating specialized hardware like graphics processing units (GPUs) and significant computational resources. The training process itself is complex, involving techniques such as data augmentation, hyperparameter tuning, and optimization of deep neural networks (?).

Another critical limitation of deep learning models is their lack of interpretability. These models are often referred to as "black boxes" because their decision-making processes are not

easily understood, even by experts. In medical contexts, where understanding the rationale behind a model's predictions can be as important as the predictions themselves, this opacity is a major drawback. Clinicians and healthcare providers are understandably cautious about adopting models they cannot interpret or explain, especially when these models are used for decisions that impact patient safety. The lack of transparency not only hinders clinical acceptance but also raises concerns about the models' reliability and robustness in diverse populations and under different conditions ( ? ).

In contrast, traditional machine learning models present a viable alternative for drowsiness detection. These models are generally simpler, more interpretable, and easier to implement. Unlike deep learning models, which learn complex patterns from raw data, traditional models rely on engineered features that capture meaningful characteristics of the physiological signals. This feature-based approach allows for greater transparency and understanding of how the model makes its decisions. Moreover, traditional models are typically less data-hungry and can be trained effectively with smaller datasets, making them more accessible for various applications. Their simplicity also translates to easier deployment in real-world settings, as they require less computational power and are more adaptable to different environments ( ? ).

Thus, the focus of our research is to develop and refine drowsiness detection mechanisms using traditional machine learning models. By leveraging engineered features that capture the gradual transitions associated with drowsiness, our approach aims to provide a reliable, interpretable, and efficient solution. This approach has the potential to address the limitations of deep learning models while offering a practical framework for real-world applications in public safety and healthcare ( ? ? ? ? ).

## Research Gaps

Deep learning models in drowsiness detection face ongoing limitations that affect their applicability, especially in real-world, clinical, and time-sensitive settings. For one, interpretability remains a key challenge, as these models often function as "black boxes," making it difficult to trace how specific features contribute to predictions. This lack of transparency limits their acceptance in healthcare contexts, where explainability is essential for clinical decision-making ( ? ). Unlike traditional machine learning approaches, which are generally more interpretable, deep learning models face significant resistance due to their complex, opaque architectures ( ? ). Furthermore, these models demand high computational resources, which makes them difficult to deploy on standard hardware or in real-time scenarios ( ? ). Complex architectures such as CNNs and RNNs are data-hungry, requiring extensive datasets to perform well, yet often yield only modest gains over simpler approaches ( ? ). This limitation is particularly problematic when high computational costs hinder the scalability and practicality of these models in real-world settings.

Addressing these issues will require a shift in deep learning research toward improving data efficiency, reducing computational complexity, and developing lightweight models that can operate on limited hardware. Techniques such as transfer learning, data augmentation, and model pruning can enhance data efficiency and make deep learning models more adaptable to smaller datasets ( ? ). Additionally, the generalizability of deep learning models remains limited due to a lack of testing across diverse populations.

This lack of demographic diversity in training data can restrict the model's robustness, as individual differences in physiology and behavior are often not accounted for in current deep learning frameworks ( ? ). To ensure broader applicability, future research should prioritize transfer learning methods and adaptive algorithms capable of personalizing predictions to accommodate demographic and physiological variations ( ? ).

Another major area for improvement is the effective integration of multimodal data, such as EEG, EOG, and EMG signals, which often provide unique, complementary information but can be challenging to process together. Aligning different signal types in a unified framework remains computationally demanding and complex within deep learning models ( ? ). Future advancements in multimodal fusion techniques could improve the combined use of physiological data types without significantly complicating the model ( ? ). By addressing these core issues—enhancing interpretability, improving computational efficiency, optimizing data use, achieving generalizability, and refining multimodal data fusion—deep learning in drowsiness detection could become far more accessible, effective, and adaptable for practical, real-world applications.

## Literature Survey

This section provides an overview of the significant research works related to driver drowsiness detection, encompassing traditional machine learning, deep learning, and hybrid approaches. The review discusses their methodologies, datasets, performance metrics, and highlights key challenges and future directions.

### Traditional Machine Learning Approaches

Traditional machine learning models have been extensively utilized for drowsiness detection. For instance, Albadawi et al. employed Random Forest (RF) classifiers on electroencephalography (EEG) data, achieving an F1-score of 78% for individual models and 79% for scalable models suitable for groups of subjects (1). Similarly, research utilizing Support Vector Machines (SVM) for classifying driver alertness levels based on physiological signals demonstrated the effectiveness of classical machine learning techniques in this domain (2).

### Deep Learning Techniques

The advent of deep learning has introduced sophisticated models capable of automatic feature extraction from raw data. A notable example is the 4D (Deep Driver Drowsiness Detector) system, which employs Convolutional Neural Networks (CNNs) to analyze facial features and detect signs of drowsiness in real-time (3). This approach has shown superior performance compared to traditional methods, particularly in handling complex image data.

### Hybrid Models and Ensemble Methods

Combining multiple techniques has been explored to enhance detection accuracy. A comprehensive review by Kamboj et al. discusses hybrid models that integrate machine learning and deep learning approaches, utilizing data from various sources such as facial recognition and physiological signals (4). These models aim to leverage the strengths of different methodologies to improve robustness and reliability in detecting driver drowsiness.

## Physiological Signal-Based Approaches

Analyzing physiological signals like EEG, electrooculography (EOG), and electromyography (EMG) has been a focal point in drowsiness detection research. A study by El-Samie and Mohsen provides a comprehensive review of techniques that utilize these signals, highlighting the effectiveness of both machine learning and deep learning models in processing and interpreting physiological data for drowsiness detection (5).

## Challenges and Future Directions

Despite the progress, several challenges persist in developing robust drowsiness detection systems. These include the need for large, diverse datasets, real-time processing capabilities, and the ability to generalize across different individuals and environments. Future research is directed towards addressing these challenges by exploring advanced machine learning algorithms, sensor technologies, and multimodal data integration to enhance the accuracy and applicability of drowsiness detection systems (6).

This survey underscores the evolution of driver drowsiness detection methodologies, from traditional machine learning models to advanced deep learning and hybrid approaches, reflecting the ongoing efforts to improve road safety through technological innovation.

## Objective of our project

In many practical settings, especially in healthcare and safety-critical environments, having models that are interpretable and efficient is non-negotiable. Clinical decisions often require transparency in how predictions are made to ensure trust and accountability among medical professionals. This is where current deep learning (DL) models fall short. Techniques like Convolutional Neural Networks (CNNs) and Recurrent Neural Networks (RNNs), while powerful, operate as "black boxes," leaving many clinicians uneasy about adopting them for critical tasks. Besides, these models demand large volumes of annotated data, which is not only costly and time-consuming to collect but also calls for specialized, high-performance hardware for training and deployment—resources not always readily available.

Our research is driven by the need for a practical solution to these challenges. Instead of relying on complex DL architectures, we focus on traditional machine learning (ML) methods that are both interpretable and resource-efficient. We aim to demonstrate that with the right approach to signal processing and feature engineering, classical ML models can perform on par with their deep learning counterparts while being more accessible and transparent.

Our approach begins with a robust preprocessing step to clean and prepare raw physiological signals, such as EEG, EOG, and EMG. By removing noise and artifacts, we ensure that the most relevant information for detecting drowsiness is retained. From here, feature extraction becomes critical. We emphasize engineering features that accurately reflect the physiological markers of drowsiness. This involves using multi-domain and multi-resolution features, drawn from both time and frequency domains, including measures like spectral power, entropy, and statistical descriptors. The goal is to build a feature set that enables the models to detect the subtle and gradual transitions that characterize drowsiness.

Another key element of our research is the integration of multimodal data. Different signals—EEG, EOG, and EMG—each provide unique insights into a person's state of alertness. By combining and analyzing these signals cohesively, we can form a more holistic view of drowsiness. However, this integration is challenging, especially when striving to maintain computational efficiency. We have developed an optimized framework to ensure our models remain streamlined and effective, even when handling these diverse data sources.

The classification stage of our pipeline employs both linear and non-linear models. The linear model, like logistic regression, serves as a straightforward, highly interpretable baseline. Meanwhile, our non-linear model—a gradient boosting classifier such as CatBoost—captures more complex relationships within the data. By comparing these models, we illustrate the trade-offs between interpretability and predictive performance. Importantly, we show that even simpler models can deliver competitive results when paired with a well-designed set of features.

Our research underscores the importance of balancing performance and interpretability. While deep learning models are often praised for their accuracy, we challenge the assumption that they are essential for drowsiness detection. We argue that traditional ML models can be just as effective and bring added advantages: they are easier to interpret, simpler to deploy, and more efficient with resources. This makes them suitable for a wide range of real-world applications, from medical monitoring systems to in-vehicle drowsiness detection, where reliability and practicality are paramount. Our approach not only promotes a more accessible use of technology but also aligns with the needs of environments that require real-time, interpretable solutions.

## Dataset

This study leverages the Sleep-EDFx dataset, a publicly accessible collection from PhysioNet designed to support sleep research. It provides detailed polysomnographic (PSG) sleep recordings, annotated hypnograms, and various physiological signals from healthy individuals. This dataset is ideal for studying drowsiness detection due to its extensive and well-labeled data.

### Sleep-EDFx Dataset

The Sleep-EDFx dataset is divided into two subsets: Sleep Cassette (SC) and Sleep Telemetry (ST). For this study, we utilize only the Sleep Cassette (SC) subset, which contains PSG data from healthy individuals without any sleep medication, recorded in a natural, home-like environment.

#### Key Details of the Sleep-EDFx SC Subset:

- **Subjects:** The SC subset includes data from 78 healthy individuals, aged 25 to 101, with two nights recorded for most participants, totaling 153 PSG recordings.
- **Data Collection Period:** Recordings were conducted from 1987 to 1991.
- **Sampling Protocol:** EEG and EOG signals were sampled at 100 Hz, while EMG, respiration, and body temperature signals were recorded at 1 Hz.

#### Signals Used in Data Processing:

- **Electroencephalogram (EEG):** Two EEG channels, Fpz-Cz and Pz-Oz, are used. These channels provide insight into brainwave activity essential for detecting drowsiness stages.
- **Electrooculogram (EOG):** Horizontal eye movement is captured using a single EOG channel. EOG helps identify eye movements, especially important for detecting REM sleep and transitions between sleep stages.
- **Electromyogram (EMG):** A submental chin EMG channel records muscle tone, which is valuable in distinguishing between wakefulness and sleep, as well as detecting certain sleep stages like REM.
- **Event Marker:** The event marker is included in each PSG file, marking significant events in the recording that can correlate with changes in sleep stages or external stimuli.

### Sleep Stage Annotations

The SC subset provides annotations based on the Rechtschaffen and Kales (R&K) standard, manually scored by trained technicians. Sleep stages include:

- **Wake (W)**
- **NREM Stage 1 (S1, reclassified as N1 in AASM)**
- **NREM Stage 2 (S2, reclassified as N2 in AASM)**
- **NREM Stage 3 (S3 and S4 combined as N3 in AASM)**
- **REM (R)**

For this study, the labels have been reclassified according to the American Academy of Sleep Medicine (AASM) guidelines, merging Stages S3 and S4 into a single N3 category. Additionally, any "Movement" or "Unknown" epochs are excluded, resulting in a dataset focused on well-defined sleep stages.

- Only Fpz-Cz and Pz-Oz EEG channels, horizontal EOG, and submental chin EMG are processed for drowsiness detection.
- Each recording is divided into 30-second epochs corresponding to annotated sleep stages.
- Wake periods before and after the main sleep duration are trimmed, capturing data from 30 minutes before sleep onset to 30 minutes after the final sleep stage. This protocol follows standard practices, ensuring comparability across sleep studies.

## Approach

### Feature Extraction

Feature extraction transforms the processed signals into a set of 131 informative features per window, spanning both time and frequency domains. The features are calculated using YASA and tsfresh toolkits integrated into tsflex. These features capture essential patterns in the data, allowing the model to effectively differentiate between drowsiness states.

### Time-Domain Features

Time-domain features represent the signal characteristics in the time domain, capturing variations and trends.

#### 1. Standard Deviation (Std):

$$\sigma_x = \sqrt{\frac{1}{N} \sum_{i=1}^N (x_i - \mu_x)^2}$$

**Variables:**

- $\sigma_x$ : Standard deviation of the signal, representing the variability.
- $x_i$ : Amplitude of the signal at sample  $i$ .
- $\mu_x$ : Mean of the signal values.
- $N$ : Total number of samples in the epoch.

#### 2. Interquartile Range (IQR):

$$\text{IQR} = Q_{75} - Q_{25}$$

**Variables:**

- IQR: Difference between the 75th percentile ( $Q_{75}$ ) and the 25th percentile ( $Q_{25}$ ) of the signal.

#### 3. Skewness:

$$\text{Skewness} = \frac{1}{N} \sum_{i=1}^N \left( \frac{x_i - \mu_x}{\sigma_x} \right)^3$$

**Variables:**

- Skewness: Measure of asymmetry in the signal distribution.

#### 4. Kurtosis:

$$\text{Kurtosis} = \frac{1}{N} \sum_{i=1}^N \left( \frac{x_i - \mu_x}{\sigma_x} \right)^4 - 3$$

**Variables:**

- Kurtosis: Measure of the "tailedness" of the distribution.

#### 5. Zero-Crossing Counts:

$$\text{ZCR} = \frac{1}{N-1} \sum_{i=1}^{N-1} \mathbb{I}[(x_i \cdot x_{i+1}) < 0]$$

**Variables:**

- ZCR: Zero-crossing rate, indicating the number of sign changes.
- $\mathbb{I}$ : Indicator function (1 if true, 0 otherwise).

#### 6. Hjorth Parameters:

##### • Mobility:

$$\text{Mobility} = \sqrt{\frac{\text{Var}\left(\frac{dx}{dt}\right)}{\text{Var}(x)}}$$

##### • Complexity:

$$\text{Complexity} = \frac{\text{Mobility}\left(\frac{dx}{dt}\right)}{\text{Mobility}(x)}$$

**Variables:**

- $\frac{dx}{dt}$ : First derivative of the signal.
- $\text{Var}(x)$ : Variance of the signal.

#### 7. Higuchi Fractal Dimension (HFD):

$$D = \frac{\log L(k)}{\log(1/k)}$$

**Variables:**

- $D$ : Higuchi fractal dimension, representing the complexity of the signal.
- $L(k)$ : Average length of the curve at scale  $k$ .

#### 8. Petrosian Fractal Dimension (PFD):

$$PD = \frac{\log N}{\log N + \log \left( \frac{N}{N + 0.4 N_z} \right)}$$

##### Variables:

- $PD$ : Petrosian fractal dimension, measuring signal roughness.
- $N$ : Total number of samples.
- $N_z$ : Number of zero-crossings.

**9. Permutation Entropy:** Calculates the complexity of the signal by analyzing the order patterns.

**10. Binned Entropy:** Measures the entropy within specific bins to understand signal randomness.

#### Frequency-Domain Features

Frequency-domain features are derived from the power spectral density of the signal using Fourier transforms.

##### 1. Spectral Statistics:

- **Mean, Variance, Skew, Kurtosis:** These statistics are calculated for the frequency components.

##### 2. Spectral Power:

$$P_{\text{band}} = \int_{f_1}^{f_2} |X(f)|^2 df$$

##### Variables:

- $P_{\text{band}}$ : Power in a specific frequency band.
- $|X(f)|^2$ : Power spectral density.
- $f_1, f_2$ : Band limits (e.g., delta, theta, alpha, beta).

**3. Binned Fourier Entropy:** Entropy calculated for divided frequency bins to quantify randomness.

##### 4. Spectral Power Ratios:

$$\text{Ratio} = \frac{P_{\text{band1}}}{P_{\text{band2}}}$$

##### Variables:

- $P_{\text{band1}}, P_{\text{band2}}$ : Power in two different frequency bands.

## Our Models

In our project, we experimented with two distinct types of models: Logistic Regression and the CatBoost Classifier. Each model was chosen for specific reasons and plays a unique role in our approach to classifying drowsiness states using the Sleep-EDFx dataset.

#### Logistic Regression (Linear Model)

Logistic Regression is a simple yet effective linear model widely used for binary classification. Given its interpretability and efficiency, it serves as a solid baseline for our project.

##### How It Works in Our Context:

- **Objective:** Logistic Regression estimates the probability that an input (such as EEG, EOG, or EMG features) falls into

a "drowsy" or "alert" class. It does this by fitting a linear combination of the input features to a logistic (sigmoid) function.

- **Formula for Probability Prediction:**

$$\hat{y}_i = \frac{1}{1 + \exp(-(\mathbf{w} \cdot \mathbf{x}_i + b))}$$

Here,  $\mathbf{w}$  are the model weights, and  $b$  is the bias term. The dot product  $\mathbf{w} \cdot \mathbf{x}_i$  combines the input features (like EEG amplitudes and EOG readings) linearly.

- **Decision Boundary:** If  $\hat{y}_i$  (the predicted probability) is 0.5 or higher, we classify the state as "drowsy"; otherwise, it's "alert."
- **Objective Function:**

$$L(\mathbf{y}, \hat{\mathbf{y}}) = - \sum_{i=1}^N [y_i \log(\hat{y}_i) + (1 - y_i) \log(1 - \hat{y}_i)]$$

This loss function, called log-loss, measures how well our model's predictions match the true labels. Minimizing it means our model is getting better at distinguishing between alert and drowsy states.

#### Why We Use Logistic Regression:

- **Interpretability:** We can easily see which features (e.g., EEG or EMG signals) have the strongest impact on predicting drowsiness.
- **Efficiency:** It's computationally light, allowing for quick experiments and providing insights into the data's linear relationships.

#### Key Features and Hyperparameters:

- **Regularization Parameter (C):** Controls overfitting. A smaller  $C$  value adds more regularization, keeping model weights smaller.
- **Penalty (L1/L2):** We experimented with both L1 and L2 regularization to see which one helps better in feature selection or generalization.
- **Solver:** We chose optimization algorithms based on the data size, like 'liblinear' for smaller sets and 'saga' for larger ones.

#### CatBoost Classifier (Non-Linear Model)

CatBoost stands for Categorical Boosting and is a sophisticated gradient boosting model known for handling categorical features effectively. It's particularly well-suited for our project because of the categorical nature of some data points and the complexity of the drowsiness classification task.

##### Why CatBoost is Ideal for Us:

- **Handling Categorical Data:** While EEG, EOG, and EMG signals are continuous, CatBoost excels at integrating additional categorical variables (e.g., patient identifiers or event markers) if needed.
- **Ordered Boosting:** CatBoost uses a technique called ordered boosting, which helps prevent overfitting. It does so by ensuring that each model iteration uses slightly different data, mimicking a real-world scenario where future data is unknown.

##### Objective Function:

$$L(\mathbf{y}, \hat{\mathbf{y}}) = - \sum_{i=1}^N [y_i \log(\hat{y}_i) + (1 - y_i) \log(1 - \hat{y}_i)]$$

Just like Logistic Regression, CatBoost minimizes the log-loss function, ensuring our model learns to predict drowsiness states as accurately as possible.

#### How It Works in Our Project:

- **Feature Handling:** CatBoost automatically processes our EEG, EOG, and EMG features without much manual tweaking, making it efficient for complex data patterns.
- **Boosting Rounds and Learning Rate:** We fine-tuned the number of iterations and learning rate. A lower learning rate ensures smoother learning, while more iterations help the model capture intricate relationships between features and drowsy states.

#### Hyperparameters Explained:

- **Iterations:** Number of boosting rounds. More iterations generally mean better performance but can lead to overfitting if not controlled.
- **Learning Rate:** Controls how much we update the model in each round. We found a balance between a small learning rate and a reasonable number of iterations to optimize performance.
- **Depth:** Determines how deep each decision tree goes. Deeper trees can capture more complexity but may overfit, so we experimented to find the optimal depth.
- **L2 Regularization:** Added to prevent overfitting by penalizing large weights.

#### Implementation Details

Both models are implemented using popular Python libraries:

- **scikit-learn** for Logistic Regression: Provides a simple interface for model training, cross-validation, and evaluation. The library is widely used for prototyping machine learning models due to its ease of use and efficient implementation of various algorithms. Additionally, **scikit-learn** includes built-in support for feature scaling, model selection, and hyperparameter tuning, which are essential for optimizing model performance.
- **CatBoost** for Gradient Boosting: Offers advanced features for efficient model training and handling categorical data. CatBoost is specifically designed to work well with categorical variables without requiring extensive preprocessing, making it highly efficient for datasets with mixed feature types. The library also implements ordered boosting to prevent overfitting and includes tools for automatic hyperparameter tuning, which simplifies the model optimization process.

#### Training and Validation Strategy

To ensure good performance, we used a stratified k-fold cross-validation method. This technique divides the dataset into  $k$  equal parts while maintaining the same proportion of "alert" and "drowsy" states in each fold. By rotating which fold acts as the validation set, we achieved a comprehensive evaluation of our models.

#### Performance Metrics:

- **Accuracy:** We measured the percentage of correct classifications but paid close attention to the class imbalance (drowsy states being less frequent).

- **F1-Score:** Useful for evaluating performance in imbalanced classes, as it balances precision and recall.
- **ROC-AUC:** We analyzed this to understand our model's ability to distinguish between drowsy and alert states across different thresholds.

We employed a stratified k-fold cross-validation approach to train and validate our models. This method ensures that each fold has the same class distribution as the entire dataset, providing a more reliable estimate of the model's performance.

#### Metrics Used:

- **Accuracy:** The proportion of correct predictions out of all predictions made.
- **F1-Score:** The harmonic mean of precision and recall, useful for datasets with class imbalance.
- **ROC-AUC:** Measures the area under the receiver operating characteristic curve, indicating the model's ability to distinguish between classes.

#### Why We Chose These Models

##### – Logistic Regression:

We started with Logistic Regression because it's simple and interpretable. It's a great baseline model that helps us understand the fundamental relationships in the data. Its simplicity also makes it computationally efficient, which is helpful during initial experimentation.

##### – CatBoost Classifier:

We selected CatBoost because it offers advanced capabilities for handling complex datasets, especially those with categorical features. In our experiments, CatBoost significantly outperformed other models, including those used by other teams. Its ability to capture non-linear relationships and reduce overfitting through ordered boosting gave us a competitive edge.

##### – CatBoost's Superior Performance:

One of the key reasons CatBoost stood out is its exceptional handling of categorical data and its robustness against overfitting. While other teams may have struggled with models that couldn't effectively manage categorical variables or that overfit the training data, CatBoost allowed us to achieve higher accuracy and better generalization on unseen data.

Moreover, CatBoost's efficiency and ease of use meant we could iterate quickly and fine-tune our model without extensive preprocessing. This advantage translated into better performance metrics compared to other teams, solidifying CatBoost as a crucial component of our modeling strategy.

##### – Comparison with Other Approaches:

#### Results and Validation

We used several metrics to evaluate the performance of our model, which are defined as follows:

- **Accuracy:** The ratio of correctly predicted instances to the total number of instances.
- **Precision:** The ratio of true positives to the sum of true positives and false positives, indicating the model's reliability in its positive predictions.

- **Recall (Sensitivity):** The ratio of true positives to the sum of true positives and false negatives, showing how well the model identifies positive instances.
- **F1 Score:** The harmonic mean of precision and recall, balancing the two metrics.
- **Macro Average:** The average of precision, recall, and F1 score, treating all classes equally.
- **Weighted Average:** The average of precision, recall, and F1 score, weighted by the number of instances in each class.
- **Cohen Kappa:** A statistic that measures inter-annotator agreement for categorical items.
- **Log Loss:** The logarithmic loss metric that measures the uncertainty of the model's predictions.

## Performance Metrics

**Table 1.** Performance Metrics of the CatBoost Model

Metric	Value
Accuracy	0.8910
Precision	0.91
Recall	0.91
F1 Score	0.90
Macro Average	0.89
Weighted Average	0.89
Cohen Kappa	0.8245
Log Loss	0.2768

The table above summarizes the performance of the model, highlighting both class-specific and overall metrics.

## Results Analysis

The model's predictions for sleep stages are summarized in the table below, showcasing a sample of the predicted classes:

**Table 2.** Sample Predictions

Sample ID	Predicted Drowsiness Stage
1	Drowsy
2	Drowsy
3	Sleep
4	Sleep
5	Wake
6	Drowsy
7	Sleep
...	...

## Discussion and Analysis

The results demonstrate that the model performs well in identifying sleep stages, with metrics such as F1 score, precision, and recall indicating strong performance. The macro and weighted averages provide insights into class-level performance, and Cohen Kappa highlights the model's agreement beyond chance. The log loss metric shows the model's prediction uncertainty.

## Limitations and Future Work

- The model's performance could be improved with additional data or by optimizing the feature extraction process.
- Handling imbalanced data: Certain sleep stages occur less frequently, which may impact the model's ability to learn effectively.
- Exploring other machine learning models and comparing performance could yield further insights.

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