Delaytools User Manual

rapidtide2

The central program in this package is rapidtide2. This is the program that quantifies the time strength and time delay of pervasive signals in a BOLD fMRI dataset.

Description:

At its core, rapidtide is simply performing a full crosscorrelation between a "probe" timecourse and every voxel in an fMRI dataset (by "full" I mean over all time lags, rather than only at zero lag, as in a Pearson correlation). As with many things, however, the devil is in the details, and so rapidtide provides a number of features which make it pretty good at this particular task. A few highlights:

- 1) There are lots of ways to do something even as simple as a cross-correlation in a nonoptimal way (not windowing, improper normalization, doing it in the time rather than frequency domain, etc.). I'm pretty sure what rapidtide does is, if not the best way, at least a very good and very fast way.
- 2) rapidtide has been optimized and profiled to speed it up quite a bit; it has an optional dependency on numba if it's installed, some of the most heavily used routines will speed up significantly due to judicious use of @jit.
- 3) The sample rate of your probe regressor and the fMRI data do not have to match rapidtide resamples the probe regressor to an integral multiple of the fMRI data rate automatically
- 4) The probe and data can be temporally prefiltered to the LFO, respiratory, or cardiac frequency band with a command line switch, or you can specify any low, high, or bandpass range you want.
- 5) The data can be spatially smoothed at runtime (so you don't have to keep smoothed versions of big datasets around). This is quite fast, so no reason not to do it this way.
- 6) rapidtide can generate a probe regressor from the global mean of the data itself no externally recorded timecourse is required. Optionally you can input both a mask of regions that you want to be included in the mean, and the voxels that you want excluded from the mean (there are situations when you might want to do one or the other or both).
- 7) Determining the significance threshold for filtered correlations where the optimal delay has been selected is nontrivial; using the conventional formulae for the significance of a correlation leads to wildly inflated p values. rapidtide estimates the spurious correlation threshold by calculating the distribution of null correlation values obtained with a shuffling procedure at the beginning of each run (the default is to use 10000 shuffled correlations), and uses this value to mask correlation maps it calculates.
- 8) rapidtide can do an iterative refinement of the probe regressor by aligning the voxel timecourses in time and regenerating the test regressor.
- 9) rapidtide fits the peak of the correlation function, so you can make fine grained distinctions between close lag times. The resolution of the time lag discrimination is set

- by the length of the timecourse, not the timestep this is a feature of correlations, not rapidtide.
- 10) Once the time delay in each voxel has been found, rapidtide outputs a 4D file of delayed probe regressors for using as voxel specific confound regressors or to estimate the strength of the probe regressor in each voxel. This regression is performed by default, but these outputs let you do it yourself if you are so inclined.
- 11) I've put a lot of effort into making the outputs as informative as possible lots of useful maps, histograms, timecourses, etc.
- 12) There are a lot of tuning parameters you can mess with if you feel the need. I've tried to make intelligent defaults so things will work well out of the box, but you have the ability to set most of the interesting parameters yourself.

Inputs:

At a minimum, rapidtide needs a Nifti file to work on (space by time), which is generally thought to be a BOLD fMRI data file. This can be Nifti1 or Nifti2; I can currently read (probably) but not write Cifti files, so if you want to use grayordinate files you need to convert them to nifti in workbench, run rapidtide, then convert back. As soon as nibabel finishes their Cifti support, I'll add that.

The file needs one time dimension and at least one spatial dimension. Internally, the array is flattened to a time by voxel array for simplicity.

Outputs:

Outputs are space or space by time Nifti files (depending on the file), and some text files containing textual information, histograms, or numbers. Output spatial dimensions and file type match the input dimensions and file type (Nifti1 in, Nifti1 out). Depending on the file type of map, there can be no time dimension, a time dimension that matches the input file, or something else, such as a time lag dimension for a correlation map.

A note on coding style:

This code has been in active development since June of 2012. This has two implications. The first is that it has been tuned and refined quite a bit over the years, with a lot of optimizations and bug fixes - most of the core routines have been tested fairly extensively to get rid of the stupidest bugs. I find new bugs all the time, but most of the showstoppers seem to be gone. The second result is that the coding style is all over the place. When I started writing this, I had just moved over from C, and it was basically a mental port of how I would write it in C, and was extremely unpythonic. Over the years, as I've gone back and added functions, I periodically get embarassed and upgrade things to a somewhat more modern coding style. I even put in some classes - that's what the cool kids do, right? But the pace of that effort has to be balanced with the fact that when I make major architectural changes, I tend to break things. So be patient with me.

Python version:

This code has been most heavily tested in python 2.7. I started slowly converting over to making it python 3 compatible once all the libraries I needed had been ported. As far as I know, the code works fine in python 3.5 - I've switched over to that on my development machine, and have not hit any version related issues in a while now. However that's no guarantee that there isn't a problem in some option I haven't bothered to test yet, so be vigilant, and please let me know if there is some issue with python 3 that I haven't caught (or any bugs, really).

Usage:

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usage: rapidtide2 fmrifilename outputname
[-r LAGMIN, LAGMAX] [-s SIGMALIMIT] [-a] [--nowindow] [-G] [-f GAUSSSIGMA] [-O
oversampfac] [-t TRvalue] [-d] [-b] [-V] [-L] [-R] [-C] [-F]
LOWERFREQ, UPPERFREQ[,LOWERSTOP, UPPERSTOP]] [-O OFFSETTIME] [-T] [-P] [-A
ORDER] [-B] [-h HISTLEN] [-i INTERPTYPE] [-I] [-Z DELAYTIME] [-N NREPS][--
refineweighting=REFINETYPE] [--refinepasses=NUMPASSES] [--
excludemask=MASKNAME] [--includemask=MASKNAME] [--lagminthresh=LAGMINTHRESH]
[--lagmaxthresh=LAGMAXTHRESH] [--ampthresh=AMPTHRESH][--
sigmathresh=SIGMATHRESH] [--refineoffset] [--pca] [--ica] [--refineupperlag]
[--refinelowerlag] [--tmask=MASKFILE][--limitoutput] [--
timerange=STARTPOINT, ENDPOINT]
[--numskip=SKIP] [--sliceorder=ORDER] [--regressorfreq=FREQ] [--
regressor=FILENAME] [--regressorstart=STARTTIME]
required arguments:
    fmrifilename - the BOLD fmri file
    outputname - the root name for the output files
preprocessing options:
    -t TRvalue - override the TR in the fMRI file with the value
                    - disable antialiasing filter
    -a
    --nodetrend
                    - disable linear trend removal
    -I
                     - invert the sign of the regressor before processing
    -i
                     - use specified interpolation type (options are 'cubic',
                       'quadratic', and 'univariate (default)')
    -0
                     - apply an offset OFFSETTIME to the lag regressors
                    - use butterworth filter for band splitting instead of
    -b
                       trapezoidal FFT filter
                     - filter data and regressors from LOWERFREQ to
    -F
UPPERFREQ.
                      LOWERSTOP and UPPERSTOP can be specified, or will be
                       calculated automatically
                     - filter data and regressors to VLF band
    -V
                     - filter data and regressors to LFO band
    -L
                     - filter data and regressors to respiratory band
    -R
                     - filter data and regressors to cardiac band
    -C
                     - estimate significance threshold by running NREPS null
    -N
                       correlations (default is 10000, set to 0 to disable)
    --nowindow
                     - disable precorrelation windowing
    -f GAUSSSIGMA
                    - spatially filter fMRI data prior to analysis using
                       GAUSSSIGMA in mm
    -M
                     - generate a global mean regressor and use that as the
                      reference regressor
                     - mean scale regressors during global mean estimation
    -m
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sliceorder Siemens	- use ORDER as slice acquisition order used (6 is	
numskip SKIP	<pre>interleave, default is 0 (do nothing)) - SKIP tr's were previously deleted during preprocessing (default is 0)</pre>	
correlation options: -O OVERSAMPFAC	 oversample the fMRI data by the following integral factor (default is 2) 	
regressor	- Read probe regressor from file FILENAME (if none specified, generate and use global regressor)	
regressorfreq	- Probe regressor in file has sample frequency FREQ (default is 1/tr)	
regressorstart	- First TR of fmri file occurs at time STARTTIME in the regressor file (default is 0.0)	
-G	- use generalized cross-correlation with phase alignment transform (GCC-PHAT) instead of correlation	
correlation fitting of -Z DELAYTIME -r LAGMIN, LAGMAX -s SIGMALIMIT	options: - don't fit the delay time - set it to DELAYTIME seconds for all voxels - limit fit to a range of lags from LAGMIN to LAGMAX - reject lag fits with linewidth wider than SIGMALIMIT	
regressor refinement options:		
refineweighting		
refinepasses	 set the number of refinement passes to NUMPASSES (default is 1) 	
includemask	 only use voxels in MASKNAME for global regressor generation and regressor refinement 	
excludemask	 do not use voxels in MASKNAME for global regressor generation and regressor refinement 	
lagminthresh	 for refinement, exclude voxels with delays less than LAGMINTHRESH (default is 1.5s) 	
lagmaxthresh	 for refinement, exclude voxels with delays greater than LAGMAXTHRESH (default is 1000s) 	
ampthresh	 for refinement, exclude voxels with correlation coefficients less than AMPTHRESH (default is 0.3) 	
sigmathresh	 for refinement, exclude voxels with widths greater than SIGMATHRESH (default is 50s) 	
refineoffset	 adjust offset time during refinement to bring peak delay to zero 	
refineupperlag refinelowerlag	 only use positive lags for regressor refinement only use negative lags for regressor refinement 	
pca	- use pca to derive refined regressor (default is	
ica	<pre>averaging) - use ica to derive refined regressor (default is averaging)</pre>	
output options:		
limitoutput -T	don't save some of the large and rarely used filessave a table of lagtimes used	
-h HISTLEN	- change the histogram length to HISTLEN (default is 100)	
timerange	- limit analysis to data between timepoints STARTPOINT and ENDPOINT in the fmri file	

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--noglm
                    - turn off GLM filtering to remove delayed regressor
                      from each voxel (disables output of rCBV)
miscellaneous options:
                    - data file is a converted CIFTI
    -c
                    - simulate a run - just report command line options
    -S
   -d
                    - display plots of interesting timecourses
experimental options (not fully tested, may not work):
   --tmask=MASKFILE - only correlate during epochs specified in
                      MASKFILE (NB: each line of MASKFILE contains the
                      time and duration of an epoch to include
                    - prewhiten and refit data
   -p
                   - save prewhitened data (turns prewhitening on)
   -P
   -A, --AR
                  - set AR model order to ORDER (default is 1)
   -B
                    - biphasic mode - match peak correlation ignoring sign
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