

# **DEI-FCTUC**

## **COMPUTATIONAL LEARNING (MEI)**

### **NEURONAL AND FUZZY COMPUTATION (MIEB)**

**2016-17**

#### **Practical work n° 3 – Prediction and detection of epileptic seizures.**

**(Theoretical content: Chaps. 6 e 7).**

Epilepsy is one of the most prevalent neurologic diseases, affecting about 1% of the population, everywhere (in Portugal about 100 000 patients). In the present state of medical knowledge about 30% of the epileptic patients are untreatable by drugs or surgery. They can suffer from a sudden seizure, anytime, anywhere, “*like a bolt from the sky*”. A seizure may last for some seconds or some minutes, and affects seriously the motor, perception, language, memory and consciousness; as a consequence, the social and professional abilities of the patients and their families are seriously diminished.

The possibility to predict or to detect a seizure, based on the information from brain signals, principally the EEG (ElectroEncephaloGram), is an actual and challenging research problem. If it would be possible to develop an algorithm to detect on time a seizure, new strategies for disarming the seizure could eventually be developed. On the other side seizure prediction would allow the patient to take action for his/her own safety and social exposition during the seizure.

An electroencephalogram is a set of electrical signals (Figure 1), in the scale of microvolts, collected by electrodes inserted inside the brain by surgery (Fig.2b) or glued to the scalp (Fig.2a).

It is supposed that many neurologic information is embedded in the EEG signals. To predict or detect a seizure, one needs to develop signal analysis methods able to detect patterns in the EEG typical of a preictal or of an ictal state, respectively.

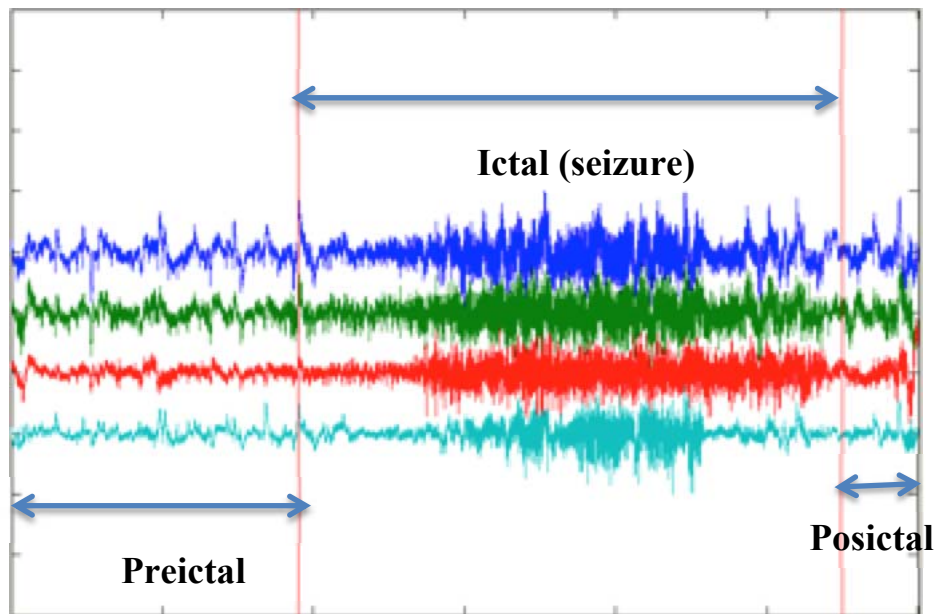


Figure 1. Electroencephalogram (EEG) with one epileptic seizure (view of 4 channels).

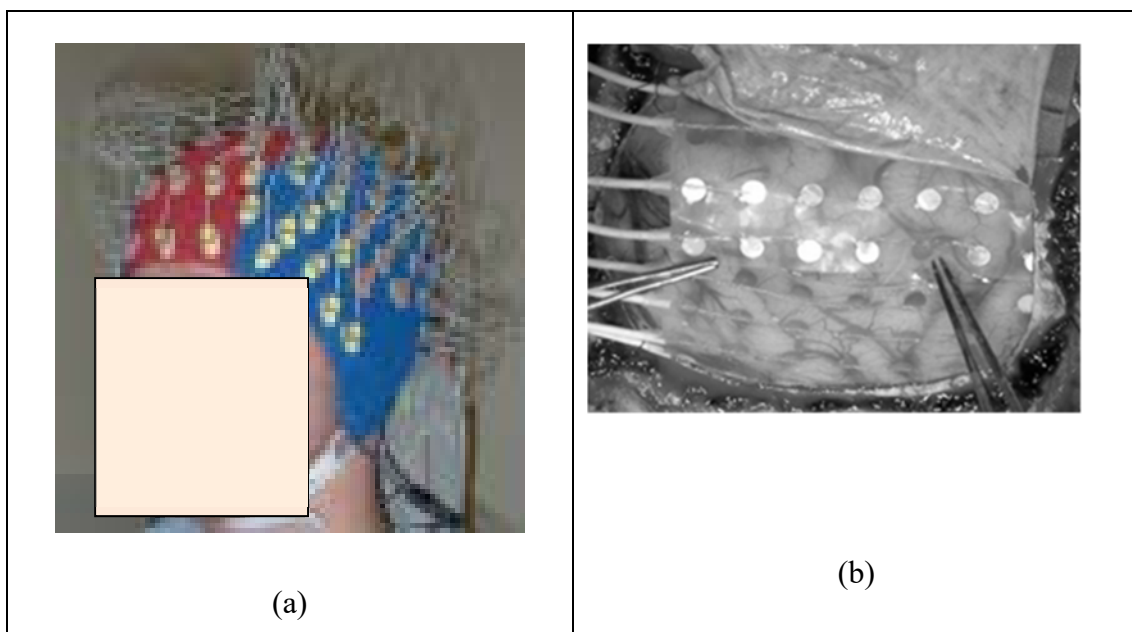


Figure 2. (a) Surface (non invasive) electrodes, (b) Intracranial (invasive) electrodes.

Each electrode feeds an EEG channel relative to an electrical reference.

In this work, for the prediction and detection of seizures, the brain state will be classified into four states. A four output NN is needed, one output for each class.

- 1- Class **inter-ictal**, corresponding to the normal brain state (output of the classifier NN 1 0 0 0).
- 2- Class **Pré-Ictal**, a seizure is coming (output of the NN 0 1 0 0).
- 3- Class **Ictal**, a seizure is happening (output of the NN 0 0 1 0).
- 4- Class **Pos-Ictal**, a seizure has just finished (output of the NN 0 0 0 1).

The 10 minutes preceding a seizure will be considered the preictal state. The 5 minutes after the seizure ended will be considered the postictal state.

The big question, previous to any classification, is to extract from the EEG a good set of features capable to distinguish the 4 classes. Although more than 30 years have passed since this question has been considered in medical and scientific fields, such a set of features has not yet been found. In the present work the set of features to be used exploit the different frequency bands of the electrical signals, and have been extracted by Doctor Mojtaba Bandarabadi, during his PhD studies in our Department. They refer to one EEG invasive channel placed in the epileptic focus (the place in the brain where the seizure starts).

The features have been extracted using 2 seconds EEG segments with 50% superposition between segments (i.e., consecutive time-windows share half of the information). In practical terms every second a vector of 29 features is obtained. These 29 features are characteristic of the frequency spectrum of the EEG channel (see at the end of this document). For the complete register of a patient, a high number of vectors is obtained, and the objective of the present work is to classify them among the defined four classes, principally to the pre-ictal and ictal classes.

The performance of the classifier is measured by the **sensitivity (how many true seizures did it preview or detect)**, high number corresponds to high sensitivity) and by the **specificity (how many false seizures did it predict or detect)**, low number corresponds to high specificity). For clinical usage, both high sensitivity and high specificity are needed. **Probably the performance is different for prediction and detection.**

The sensitivity (for prediction or for detection) is defined by

$$SE = Sensitivity = \frac{True\_Positives}{True\_Positives + False\_negatives} = \frac{TP}{TP + FN}$$

And the specificity (for prediction or for detection) is

$$SP = \text{Specificity} = \frac{\text{True\_Negatives}}{\text{True\_Negatives} + \text{False\_positives}} = \frac{TN}{TN + FP}$$

Features from 11 patients have been kindly extracted by Doctor Mojtaba Bandarabadi (we thank and acknowledge him for that).

Data from two patients will be given to each group.

The following challenge is proposed:

- Build and train NNs with the best success, one in predicting and another in detecting (it is very unlikely that one will be good for both, but you can try).

The training and testing datasets must have the usual properties, so they must include seizures. If you use validation, the validation set must also have seizures. If your patients do not have enough seizures for training, validation and testing, consider only training and testing. For example, for a patient with 9 seizures, you may use 70% (6 seizures) for training and 30% (3 seizures) for testing. Use indexes to divide the dataset in training, validation and testing, since the data must be temporarily ordered, except in the training data when class balancing is made (see Note 3).

Take full freedom to chose your NN, even if it is outside of those studied in the class.

The report must describe in detail each used NN: type, number of layers, number of neurons per layer, activation function, learning and training function. Etc.

Some remarks:

## 1 – Choosing the architecture

In a first approach one can use a normal feedforward NN (with the command `newfeedforward`). However, considering that the brain is a dynamical system, it has memory, and as such it will be interesting to face the possibility to introduce delays in some features, or in some layers. For example, the layer Recurrent Network can be used:

`net=layrecnet(layerDelays,hiddenSizes,trainFcn)` (see help in Matlab)

In this architecture, the output of each layer is fed back, with one delay, to the input of the same layer. RBF NN can also be used. These architectures are available in the *nnntool* GUI and the toolbox has appropriate training algorithms for them.

**2 –GUI for the work.** To make the study the GUI called by *nntool* in the command line can be used.

The final application to be developed by each group must have a GUI for:

- choice of the of the NN to be trained and tested
- choice of a NN already trained that is accessible to the user
- selection of the datasets (for training and testing, and also for validation if it is used)
- presentation of the results of training and of testing, with the computed sensitivity and specificity showed in the GUI.

The *guide* can be used to built the GUI. It allows to develop quickly and easily any GUI. Just type *guide* in the command line. There is an online manual for *guide*.

### 3. Building the training and testing sets.

One important issues in problems involving the detection of rare events, as it is the case of seizures, is the short duration of an event compared to the long duration without events.

In the present case, a seizure may last in average 90 seconds, while the average registered time per patient is 162 hours. From the classification point of view this means that the number of data points for the ictal class is much lower that for the other classes, specially the interictal class that contains more than 90% of the points. Without some precaution, the results can be good if the NN classifies well all the interictal points and classifies wrongly all the ictal (or preictal) points. This means, a good result, from the point of view of statistics, but a catastrophic result from the point of view of the aim of the problem.

One common way of preventing this effect, is to equilibrate the number of points of the several classes in the training set, but not in the testing set. This is the class balancing approach.

For a patient, a number of interictal points at most equal to the sum of the points of the other classes should be chosen, for example randomly. This corresponds to an undersampling of the interictal phase.

Moreover, even with (or without) class balancing, it may be interesting to give more importance to the ictal (for detection) or preictal (for prediction) instants. This may be

done by the use of different penalizations of the error of the NN in the different instants. See the toolbox User's Guide, page 4-43.

Without class balancing, if for example there are 1000 more interictal instants than ictal ones, then the weights of the errors in ictal instants should be at least 1000 greater than the weights of the interictal instants. Even with class balancing better results can be expected if the weights for preictal (prediction) or ictal (detection) are higher. Let us say that an adequate choice of the weights "specializes" the network for the class with higher weights.

#### 4- The supplied datasets have the following variables inside:

- **FeatVectSel**: Features matrix, where each column represents an extracted feature, and each row a vector of features. So this matrix must be transposed to make the **P** matrix defined in classes.
- **Trg**: A column matrix that identifies the seizures. It is made with 0's and 1's. The value 0 means non-ictal class (so interictal, preictal, or postictal), and the value 1 ictal.
- The points of the **preictal** are easily defined: 600 points before the first 1 for each seizure, corresponding to 600 seconds=10 minutes. Similarly, the **postictal** points are those 300 after the last 1 of each seizure (5 minutes).
- The **Trg vector must be changed** to identify all the four classes. For example 1 for interictal, 2 for preictal, 3 for ictal, 4 for postictal.
- After that, the **target matrix T defined in the classes must be built in accordance to the changed Trg**. Using the suggested values, the points 1 in Trg correspond to [1 0 0 0]' in T, the points 2 in Trg to [0 1 0 0]' in T, the 3 to [0 0 1 0] in T, and the 4 to [0 0 0 1]' in T.

#### 5- Postprocessing:

In an initial approach, one classifies point by point, i.e., each point must be assigned by the classifier to one of the four classes. The errors and the performance are computed point by point.

In a more elaborated approach, one may consider the following hypothesis: a seizure is predicted only if, for example, one finds 10 consecutive points classified as preictal, and

a seizure is detected only if the classifier finds 10 consecutive ictal points. However, a more relaxed hypothesis can be followed, and instead of 10 consecutive one may accept 5 among the last 10 points as a tentative threshold.

If one group wants to test in more than two patients, just ask for more data.

## 6. Remark about the used features.

The information given by the frequency content of the EEG signals is considered indicative of the brain state: different states produce different spectra, meaning that the energy of the signal is distributed among the several frequencies depending on the brain state.

The spectra measure the contribution of each frequency for the total energy of the system. The spectral power of a frequency band is given by the sum of the powers of each frequency in the band. It is supposed that the distributions of the spectral powers are different in the four considered states.

In the present study are used, by empiric choice, the normalized power spectra (in such a way that their average is null and variance is unit) of the following 29 frequency (Hz) bands, covering the total band of 0.5 to 512 Hz:

0.5-3, 3-5, 5-8, 8-10, 10-12, 12-14, 14-16, 16-18, 18-22, 22-26, 26-30, 30-35, 35-40, 40-48, 52-60, 60-70, 70-80, 80-90, 90-98, 102-125, 125-148, 152-175, 175-198, 202-248, 252-298, 302-348, 352-398, 402-512, 0.5-512Hz.

## 7. Details about the patients (from The European Epilepsy Database, built by the European Project FP7 EPILEPSIAE, [www.epilepsiae.eu](http://www.epilepsiae.eu) ).

ID	Sex	Patient age (y)	Onset age (y)	Localization of seizures	Seizure type	Total EEG Recording (h)	No. of seizure	Seizure duration (s)		
								Mean	Min	Max
107702	F	29	10	RMT, RLT	CP(1), SP(7), UC(1)	183	9	82.3	13	172
109602	F	32	1	LMT	CP(8), UC(1)	162.6	9	121.9	74	157
112502	F	11	3	RMT	CP(4), SP(4), UC(6)	155	14	122.7	56	171
115002	F	32	8	RBF, RMT, LMT	CP(2), SP(2), UC(5)	151.6	9	122.5	38	210
132502	F	18	6	L-T, L-F	CP(13)	127.8	13	86.5	68	105
44202	M	21	5	RLT, RMT	CP(19), UC(3)	170.6	22	131.6	19	199
54802	M	17	1	LMT, LLT, L-T	SP(25), SG(6)	142	31	118.4	33	274
59002	M	18	11	LBT, LLT, RBT	CP(4), SP(4), SG(4), UC(1)	246.2	13	100.2	36	137

63502	F	63	30	LMT, R-T	CP(15), UC(4)	118.9	19	102.8	8	156
92202	M	39	8	L-F, L-C	CP(2), SP(3), UC(25)	110.6	30	15.4	6	43
95802	F	14	13	L-T, LLT	CP(6), SG(4), UC(4)	217.1	14	52.5	7	123
Sum	7F/4M	-	-	-	CP(74), SP(45), SG(14), UC(50)	1785.4	183	-	-	-
Mean	-	26.7	8.7	-	-	162.3	16.6	91.8	32.5	158.8

- ❖ Localization of seizures: ABC; A (R: right, L: left), B (-: none, B: basal, L: lateral, M: mesial), C (F: frontal, T: temporal, C: central).  
E.g. RMT (right mesial temporal lobe), L-F (left frontal lobe), RBF (right basal frontal lobe).
- ❖ Seizure type: type of the clinical seizures; CP: Complex Partial, SP: Simple Partial, SG: Secondly Generalized, UC: Unclassified.  
The numbers given in parentheses represent the number of seizures for each type.
- ❖ Seizure duration: mean, minimum, and maximum values of seizure durations, considering electrographic onsets and offsets of the seizures.

Wishing you a nice work. 12/10/2016.